

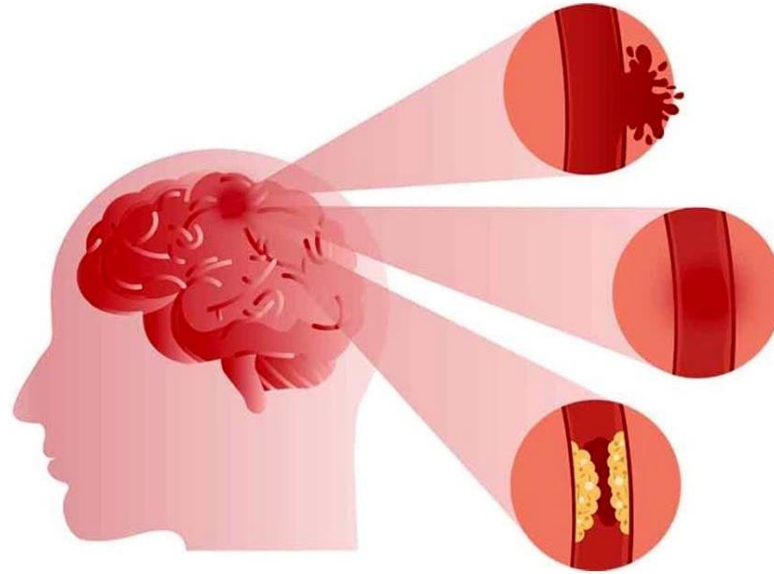
Medical/Bio Research Topics II: Week 06 (08.10.2024)

# Practical Implementation of AI Models for Segmentation (1): Dataset Exploration and Problem Formulation

분할 인공지능 모델 개발 실습 (1): 데이터 및 예측 문제

# Stroke

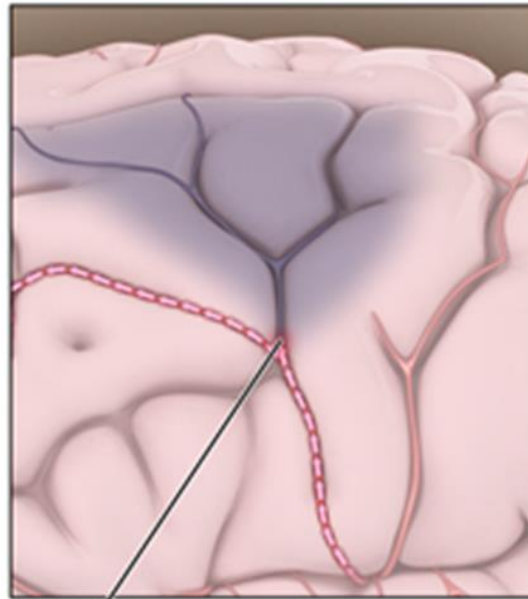
- Medical condition in which poor blood flow to the brain causes cell death



[<https://mewarhospitals.com/stroke-causes-symptoms-and-treatment/>]

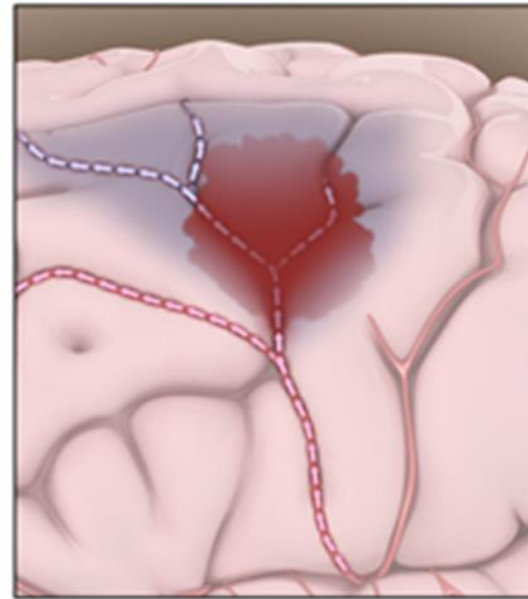
- Two types of stroke
  - Ischemic ('ischein' (to restrain) + 'haima' (blood)) stroke
    - Most common type of stroke
    - State where blood supply to a specific area is reduced or blocked
    - The brain cannot get oxygen and nutrients from the blood, so that brain cells begin to die within minutes
  - Hemorrhagic ('haima' (blood) + 'rhegnynai' (to burst forth)) stroke
    - State where a blood vessel has ruptured, causing bleeding
    - The leaked blood results in pressure on brain cells, damaging them

Ischemic stroke



A clot blocking blood flow  
to an area of the brain

Hemorrhagic stroke



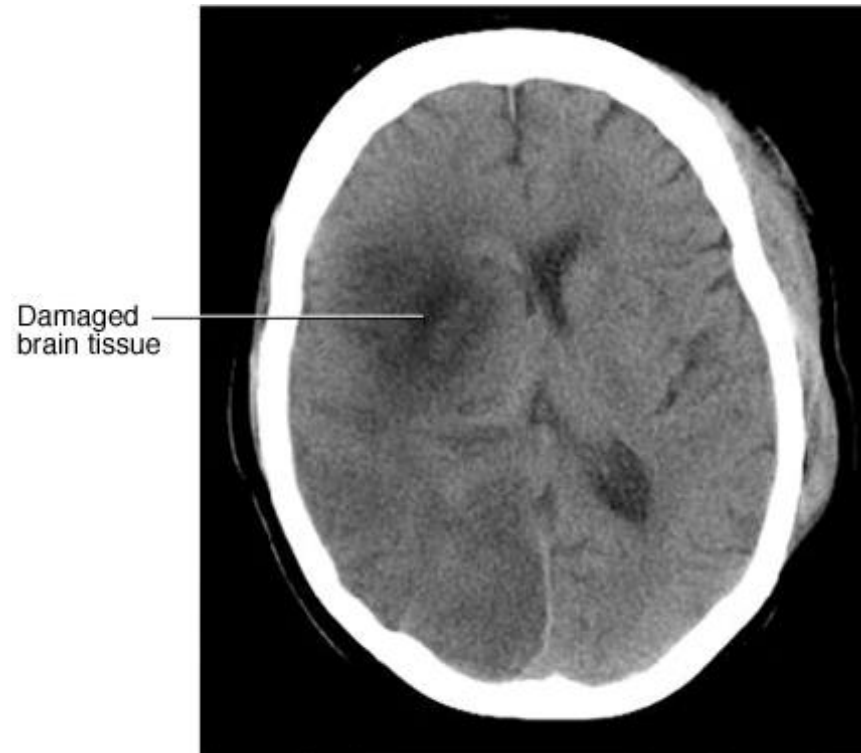
Bleeding inside or around  
brain tissue

[\[https://myhealth.alberta.ca/Health/Pages/conditions.aspx?hwid=tp12720\]](https://myhealth.alberta.ca/Health/Pages/conditions.aspx?hwid=tp12720)

## Ischemic vs. hemorrhagic stroke

- Medical emergency
  - Signs and symptoms
    - Trouble speaking and understanding what others are saying
    - Paralysis or numbness of the face, arm, or leg
    - Problems seeing in one or both eyes
    - Headache
    - Trouble walking
  - Early treatment can reduce brain damage and other complications

- Diagnosis
  - Determines the type of stroke
  - Rules out other possible causes of symptoms
  - Tests
    - Physical exam
    - Blood tests
    - CT
    - MRI



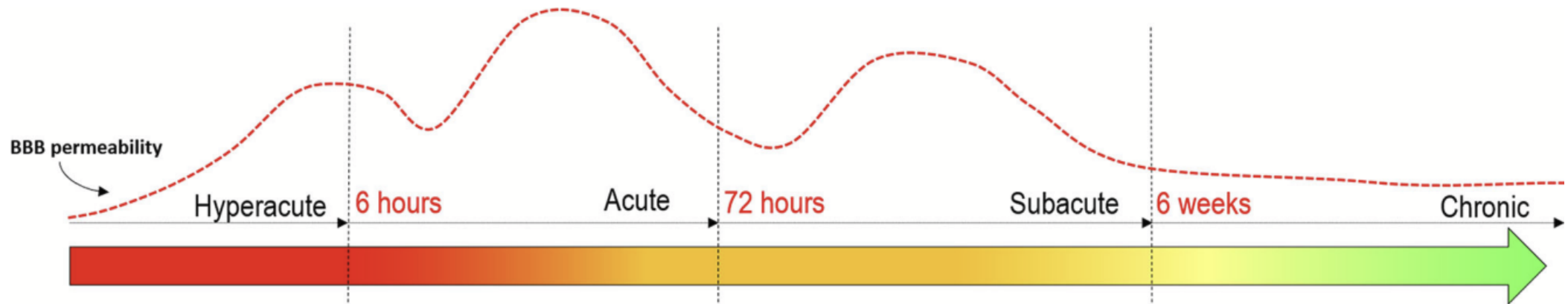
[\[https://www.mayoclinic.org/diseases-conditions/stroke/diagnosis-treatment/drc-20350119\]](https://www.mayoclinic.org/diseases-conditions/stroke/diagnosis-treatment/drc-20350119)

**CT scan of brain tissue damaged by stroke**

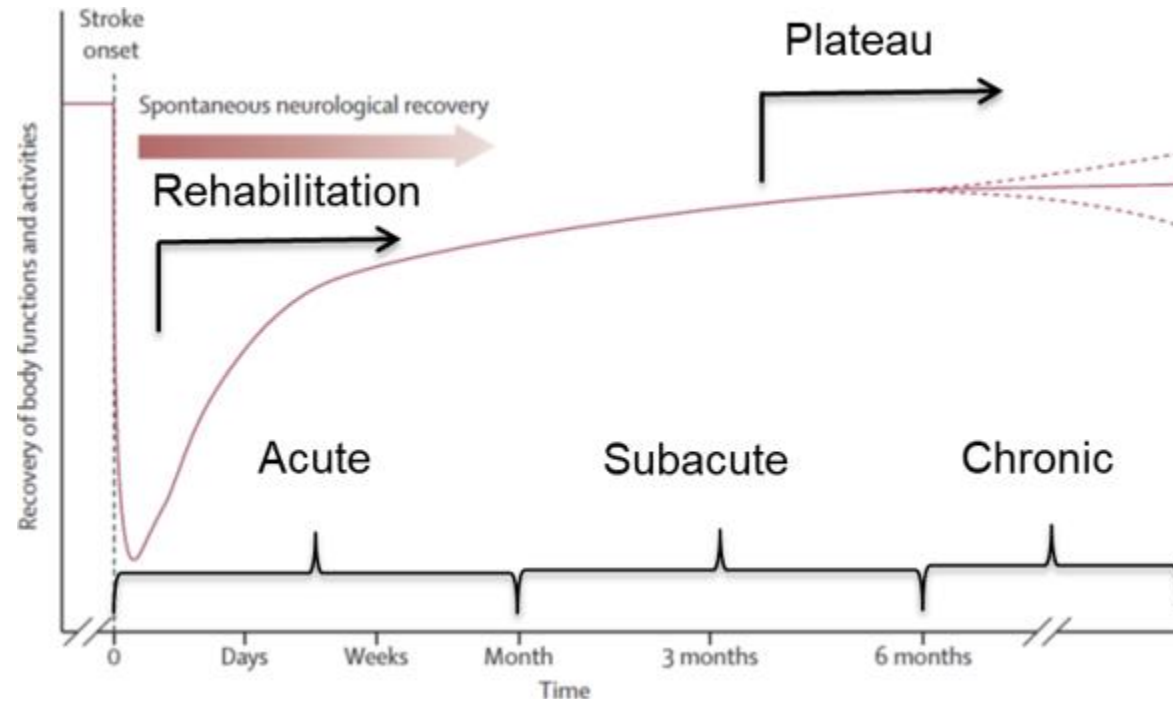
- Emergency treatment
  - Depends on the type of stroke
  - Ischemic stroke
    - Intravenous injection of recombinant tissue plasminogen activator (TPA) to dissolve the blood clot
      - Usually given through a vein in the arm within the first three hours
    - Endovascular therapy to directly remove the blood clot
  - Hemorrhagic stroke
    - Surgery to remove the blood and relieve pressure on the brain
    - Endovascular therapy to cause blood to clot



- Stages of stroke
  - Acute phase: hours to days after onset
  - Subacute phase: days to weeks
  - Chronic phase: weeks onwards



- Rehabilitation therapy
  - For most stroke survivors depending on the area of the brain involved and the amount of tissue damaged
  - Focuses on helping to recover as much function as possible and return to independent living
  - May begin before discharge and continue after discharge in a rehabilitation unit, as an outpatient, or at home
  - After getting proper treatment during stroke attacks, most of the neurological recovery happens within 3-6 months
    - Most commonly, a stroke recovery plateau occurs around 3-6 months after stroke, in which little or no gains in function happen



[Sharif et al., 2022]

## Stroke recovery plateau

- Proportional recovery rule

- The degree of natural recovery up to a stroke recovery plateau is proportional to initial functional impairment [\[Winters et al., 2015\]](#)

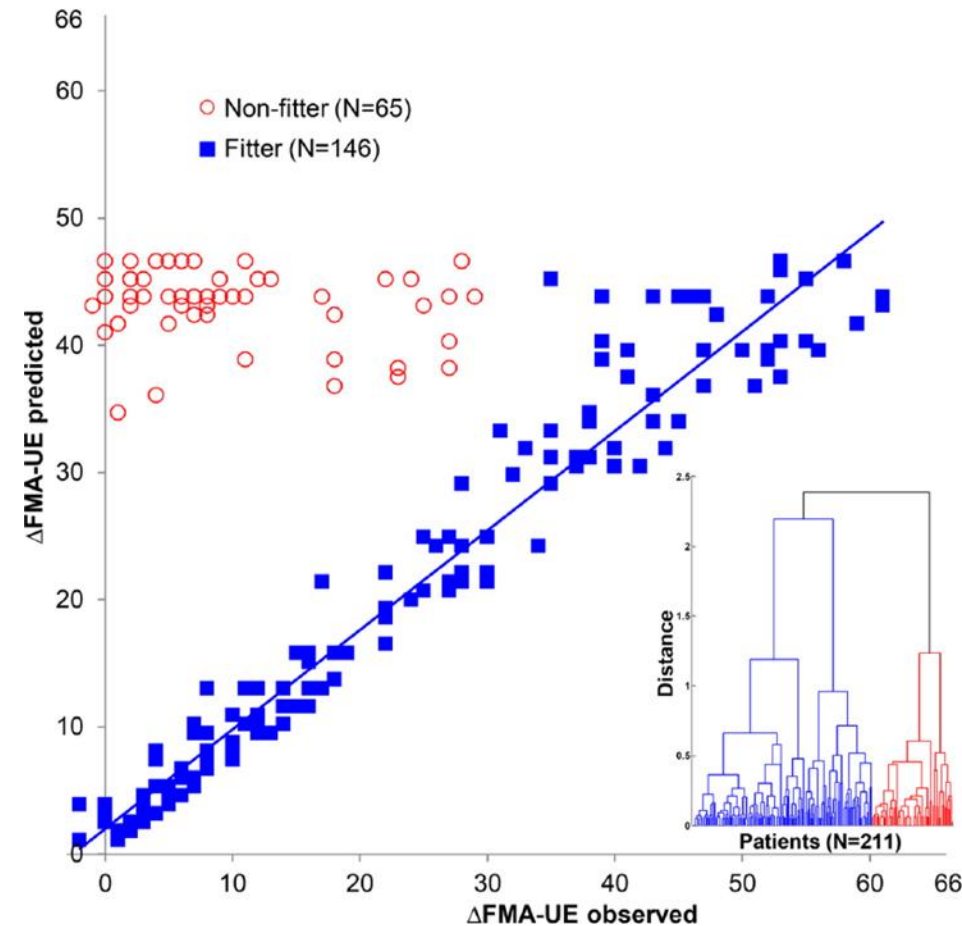
$$\begin{array}{l} \text{Predicted recovery} \qquad \qquad \qquad \text{Potential recovery} \\ \Delta \text{FMA} - \text{UE}_{\text{predicted}} = 0.7 \cdot (66 - \text{FMA} - \text{UE}_{\text{initial}}) + 0.4 \\ \approx 0.7 \cdot (\text{maximal potential recovery}) \end{array}$$

FMA-UE, Fugl-Meyer assessment of the upper extremity

- Applied to different functional domains including upper and lower limb motor, aphasia, and neglect

$$\Delta\text{FMA-UE}_{\text{observed}} = \text{FMA-UE}_{6\text{months}} - \text{FMA-UE}_{\text{initial}}$$

$$\Delta\text{FMA-UE}_{\text{predicted}} = 0.7 \times (66 - \text{FMA-UE}_{\text{initial}}) + 0.4$$

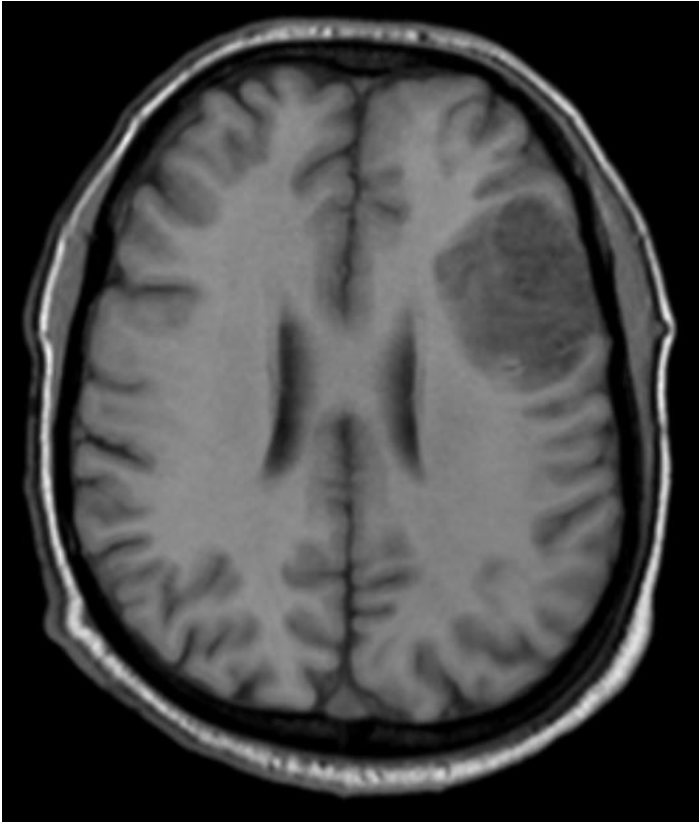


[Winters et al., 2015]

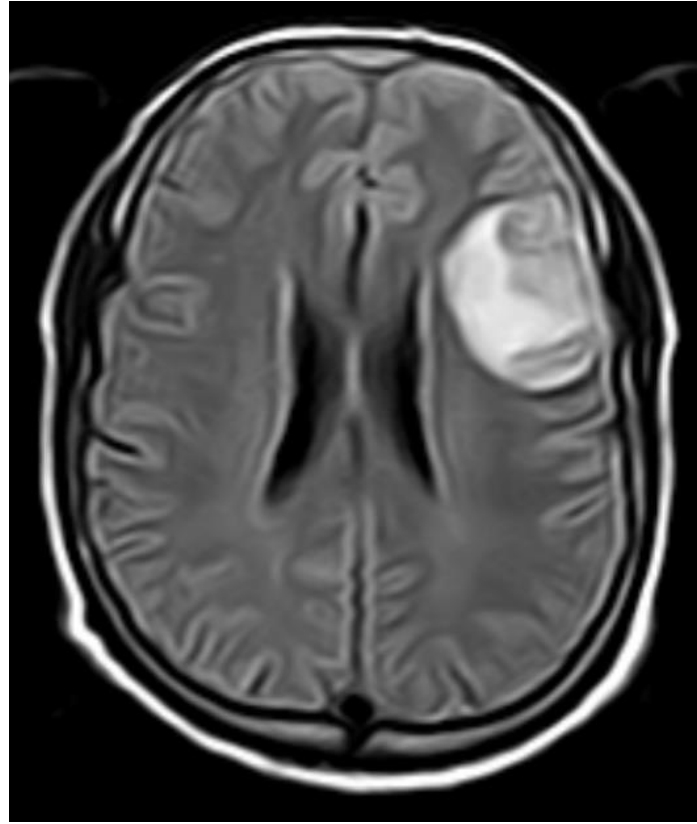
**Proportional motor improvement in the upper limb**

# Stroke Lesion

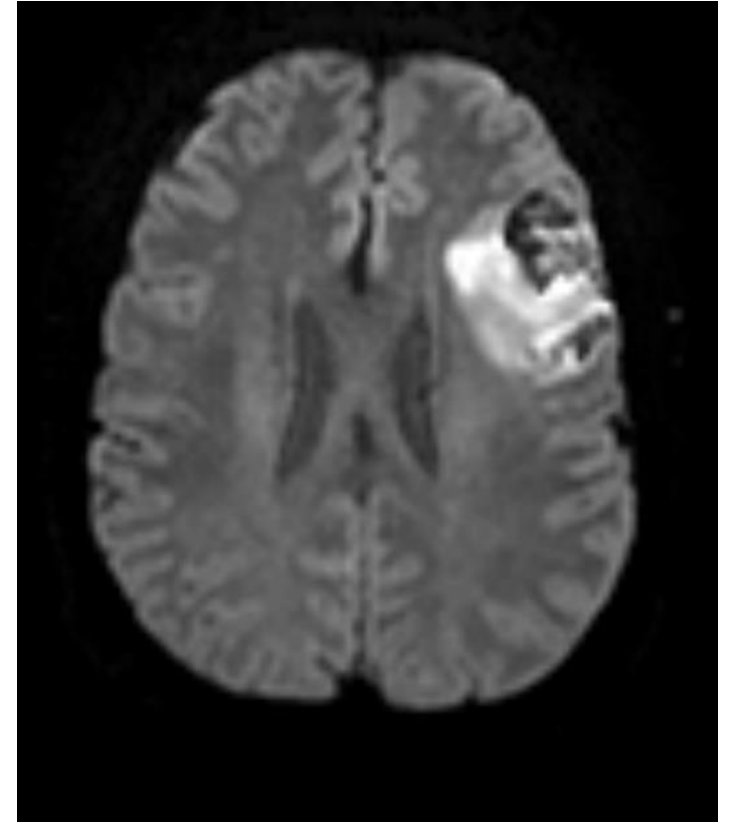
- Ischemic lesion
  - Acute ischemic lesion
  - Subacute/chronic infarct (permanent tissue damage)
- Hemorrhagic lesion
  - Intracerebral hemorrhage (ICH)
  - Subarachnoid hemorrhage (SAH)



T1-weighted



FLAIR

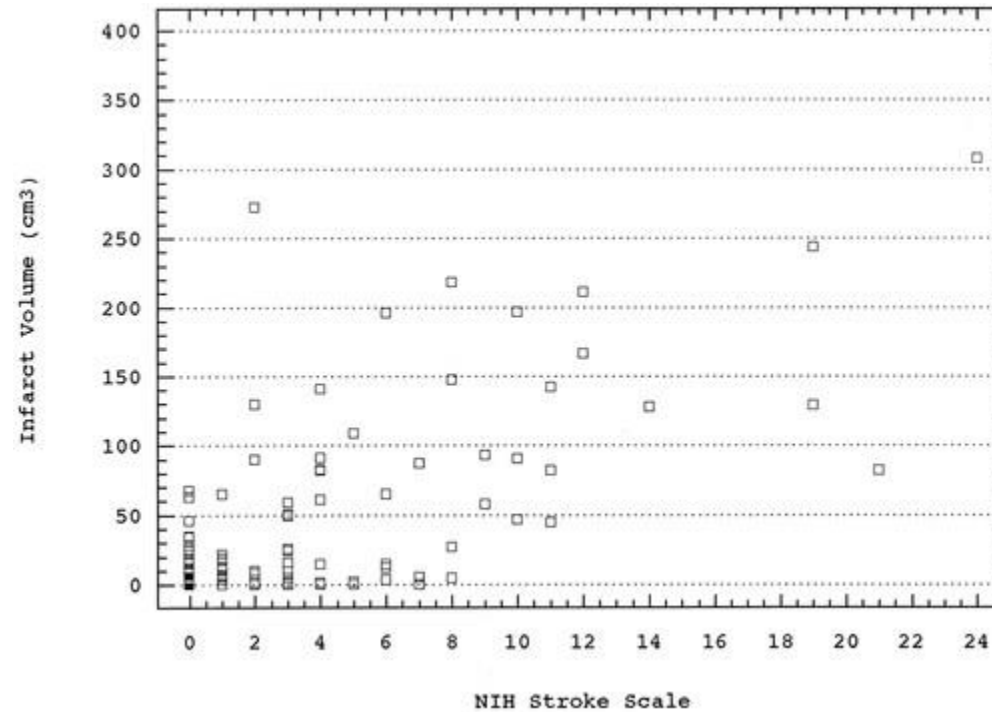


Diffusion-weighted

[\[https://www.mayoclinic.org/diseases-conditions/stroke/diagnosis-treatment/drc-20350119\]](https://www.mayoclinic.org/diseases-conditions/stroke/diagnosis-treatment/drc-20350119)

**Stroke lesion displayed as altered signals in MRI**

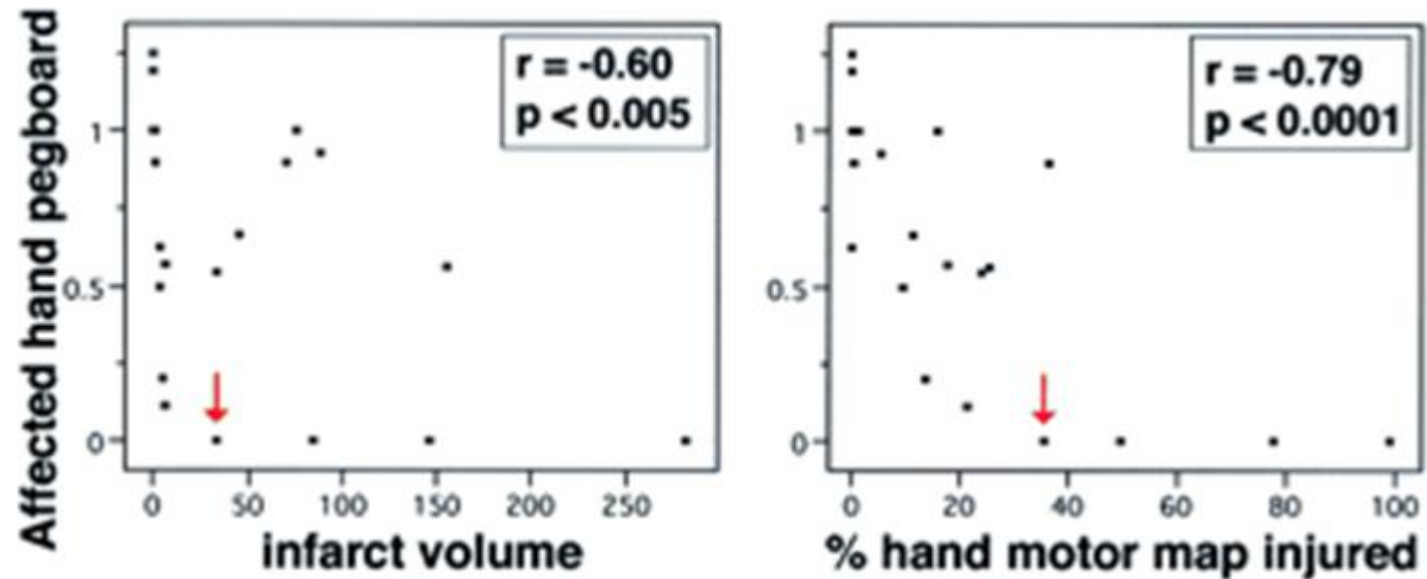
- Brain-behaviour relationship in stroke rehabilitation
  - Lesion size
    - Lesion volume correlates with clinical outcome





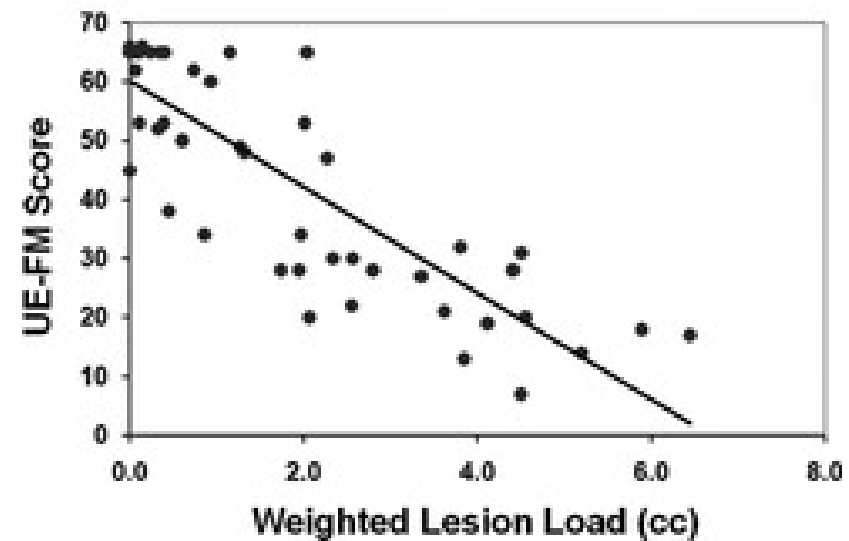
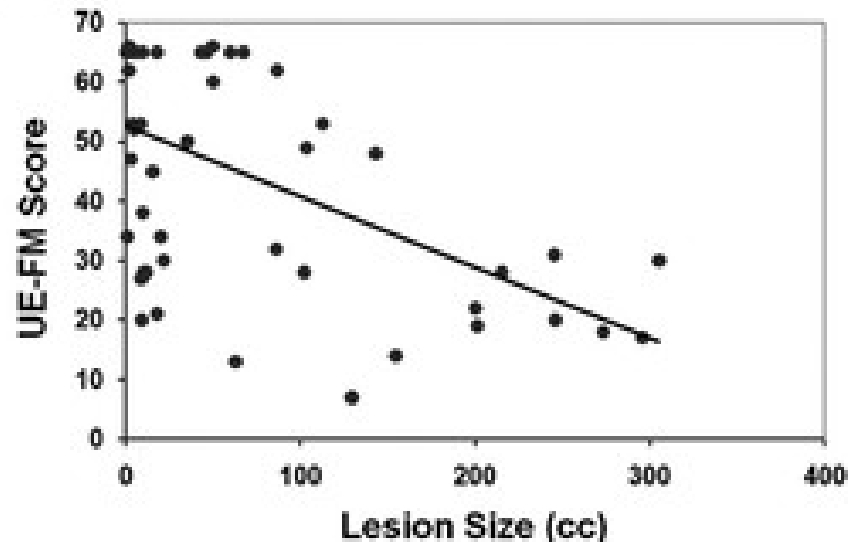
## – Lesion location

- Motor performance correlates with the fraction of hand motor map injured more strongly than with lesion volume

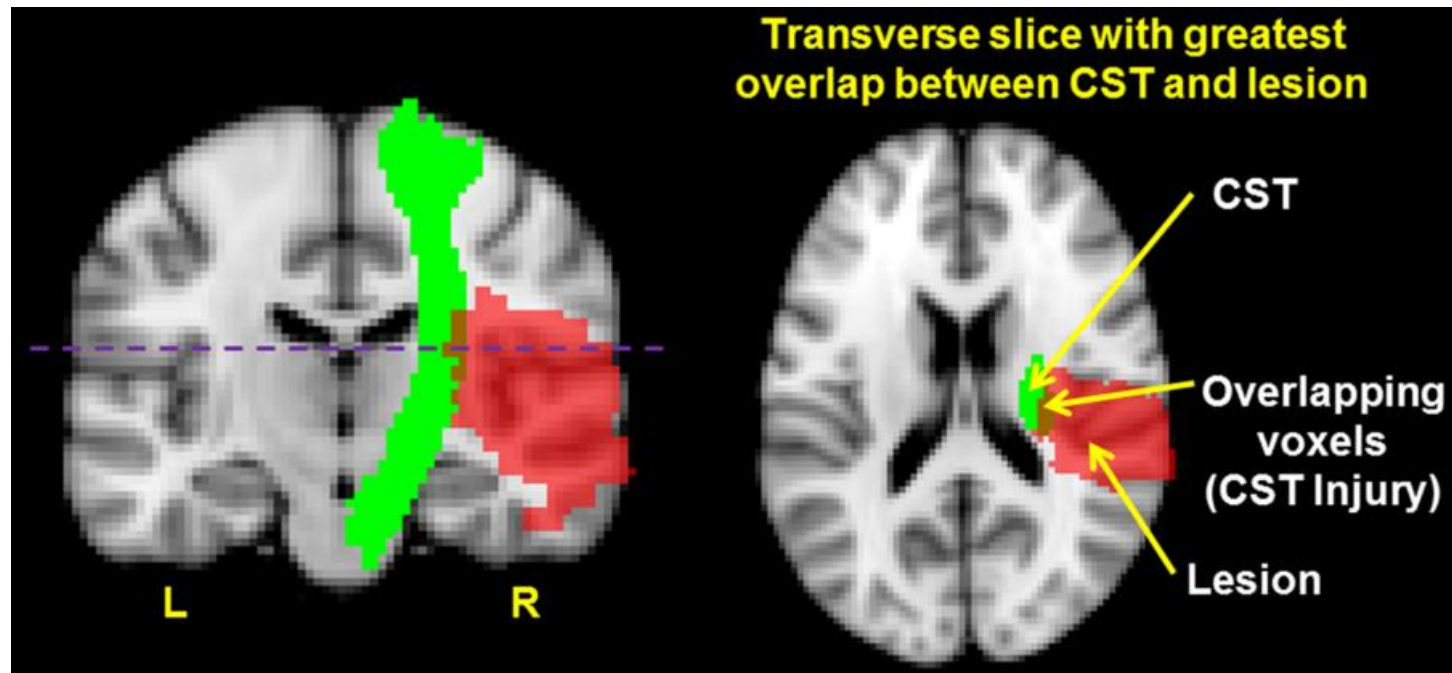


[Crafton et al., 2003]

- Lesion load: lesion overlap with extant brain structures
  - Motor impairment correlates with the proportion of the corticospinal tract injured more strongly than with lesion volume



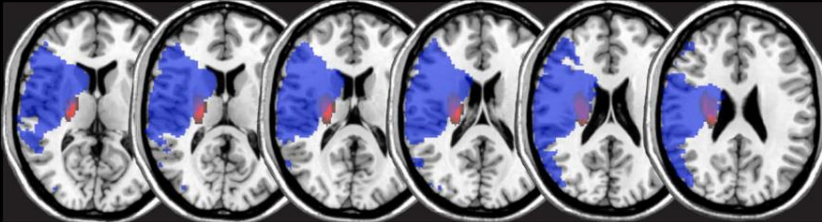
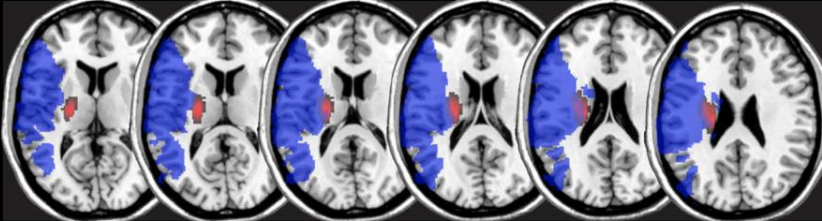
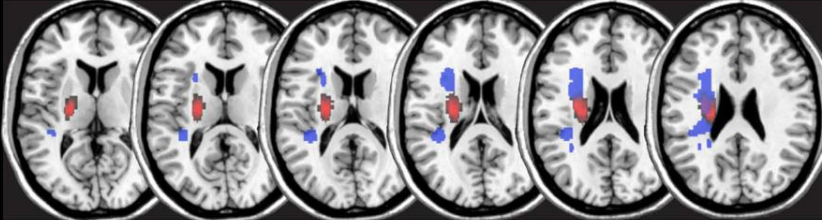
$$\text{CST Injury} = \left( \frac{\text{Number of overlapping voxels between the CST and lesion for the transverse slice}}{\text{Total number of CST voxels for the transverse slice}} \right) \times 100\%$$



[Lam et al., 2020]

**Computation of corticospinal tract lesion load**

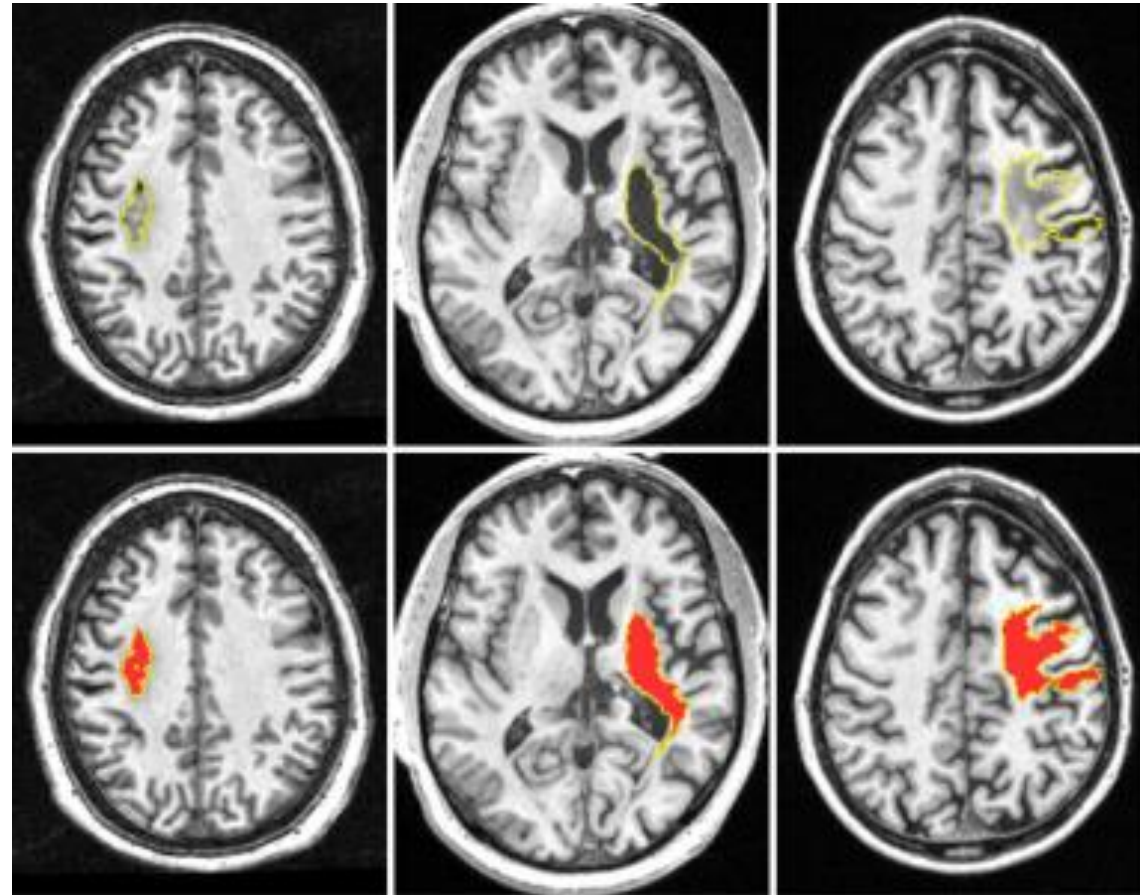
- Corticospinal tract lesion load can predict motor outcome

Patients	FM-UE		NIHSS		Lesion Size (cc)	Weighted Lesion Load (cc)
	Pre	Post	Pre	Post		
A	8	8	18	11	149	9.19
						
B	11	65	13	1	143.81	4.38
						
C	8	12	18	6	20.01	7.45
						

[Feng et al., 2015]

# Lesion Segmentation

- Critical in stroke rehabilitation research
  - For the quantification of lesion burden
  - For accurate image processing
- Still faces challenges and difficulties primarily due to variations of lesions in terms of shape, size, and location
- Manual segmentation remains the gold standard, but it is time-consuming, subjective, and requires neuroanatomical expertise



[Wu et al., 2023]

**Variations of stroke lesions**

- Anatomical Tracings of Lesions After Stroke (ATLAS) v2.0 dataset [\[https://fcon\\_1000.projects.nitrc.org/indi/retro/atlas.html\]](https://fcon_1000.projects.nitrc.org/indi/retro/atlas.html)
  - Primarily led by the Mark and Mary Stevens Neuroimaging and Informatics Institute at the University of Southern California (USC)
  - Released in 2021 by expanding upon and replacing ATLAS v1.2 released in 2018
  - Largest dataset of its kind
  - Intended to be a resource for the scientific community to develop more accurate lesion segmentation algorithms
  - Derived from diverse, multi-site data from 44 research cohorts worldwide

- Includes T1-weighted MRI scans and manually segmented lesion masks ( $n = 1,271$ )
  - Training and test sets derived from 33 research cohorts
    - Samples from each research cohort are randomly assigned to either training or test sets so that they have similar compositions
    - Training set ( $n = 655$ ): publicly released T1-weighted MRI scans and lesion masks
    - Test set ( $n = 300$ ): publicly released T1-weighted MRI scans and hidden lesion masks
  - Generalizability set derived from 11 new cohorts
    - To test the performance of trained algorithms on completely unseen data
    - Generalizability set ( $n = 316$ ): completely hidden T1-weighted MRI scans and lesion masks from separate cohorts



## – T1-weighted MRI data

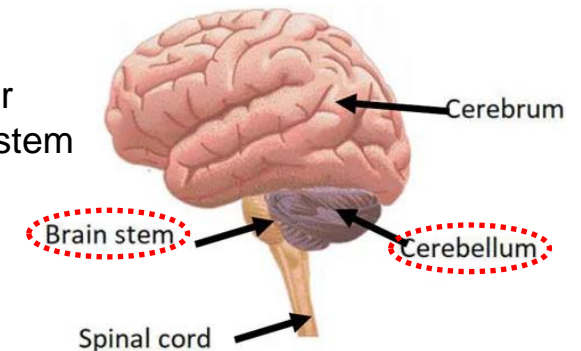
- Collected on 1.5 Tesla and 3 Tesla MR scanners
  - Each cohort was collected on a single scanner using the same parameters except for 2 cohorts
- High-resolution with the voxel size of 1 mm<sup>3</sup> or higher

## – Lesion masks [\[Liew et al., 2022\]](#)

- Number of lesions and lesion location were manually recorded

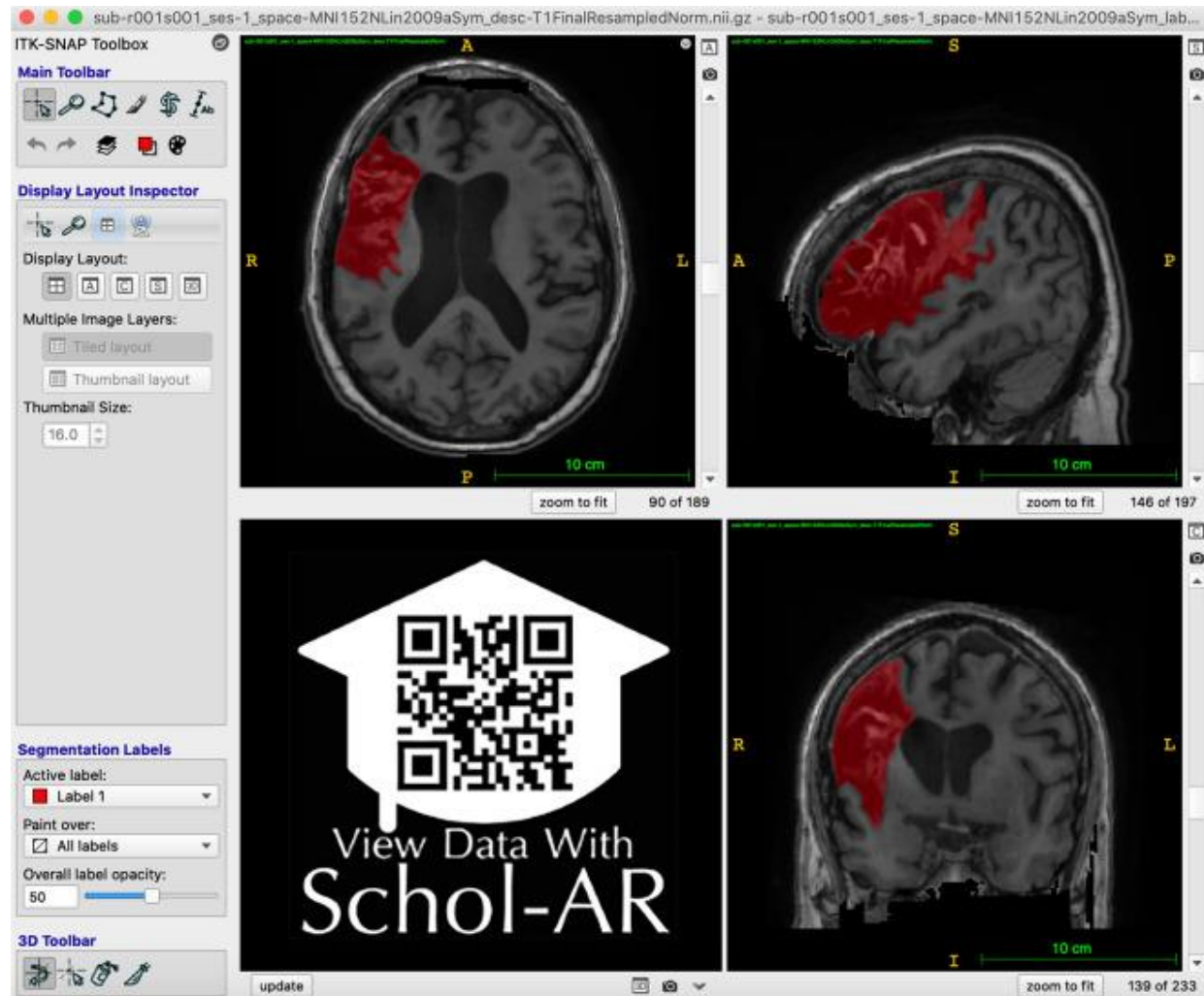
	Subjects with One Lesion			Subjects with Multiple Lesions		
	Left	Right	Other	Unilateral	Bilateral	Other
Training data (n = 655)	173 (26.4%)	187 (28.5%)	46 (7.0%)	47 (7.2%)	121 (18.5%)	81 (12.4%)
Testing data (n = 300)	88 (29.3%)	95 (31.7%)	23 (7.7%)	16 (5.3%)	43 (14.3%)	35 (11.7%)

Located In either  
cerebellum or brainstem



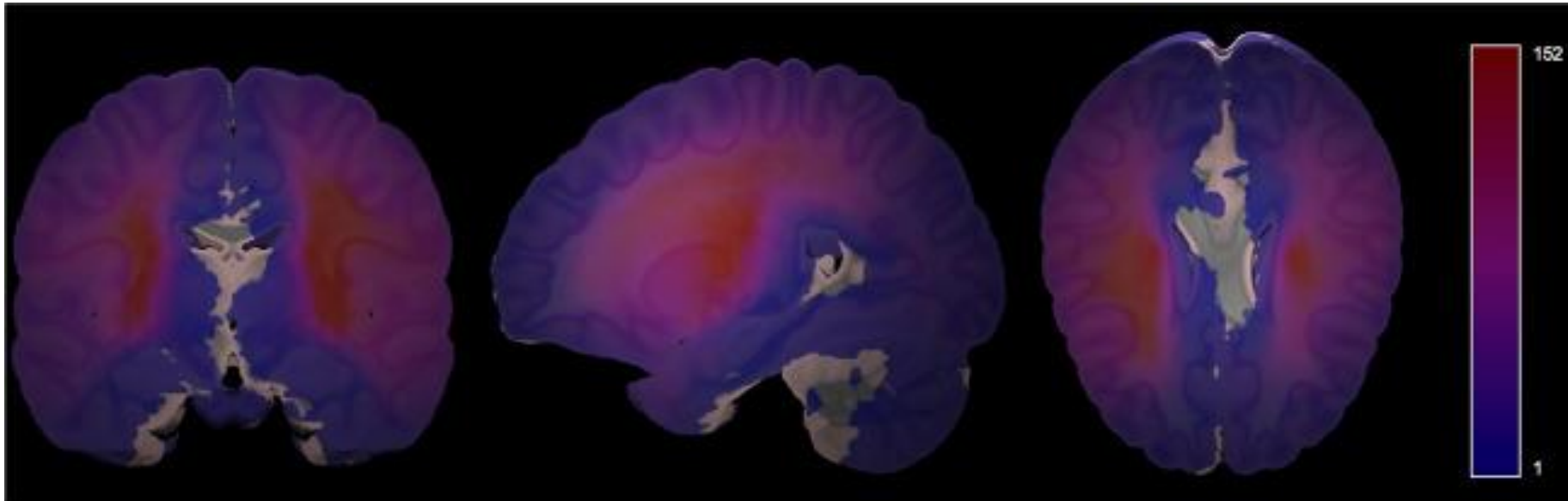
## – Lesion identification and manual tracing

- By using ITK-SNAP [\[http://www.itksnap.org/\]](http://www.itksnap.org/)
- White matter hyperintensities of presumed vascular origin and perivascular spaces were excluded from lesion masks as much as possible
- All identified lesions for each subject were reviewed for quality control by two additional trained raters



[Liew et al., 2022]

## Manual lesion segmentation in ITK-SNAP



[Liew et al., 2022]

**Lesion overlap across all subjects ( $n = 955$ ) overlaid on the MNI template brain**

# Image Segmentation

- Technique in digital image processing and analysis to partition an image into multiple parts or areas, often based on the characteristics of the pixels/voxels in the image
  - Involves converting an image into a collection of regions of pixels/voxels that are represented by a mask or a labeled image
- A common application in medical imaging is to detect and label pixels/voxels that represent an abnormality in the brain or other organs

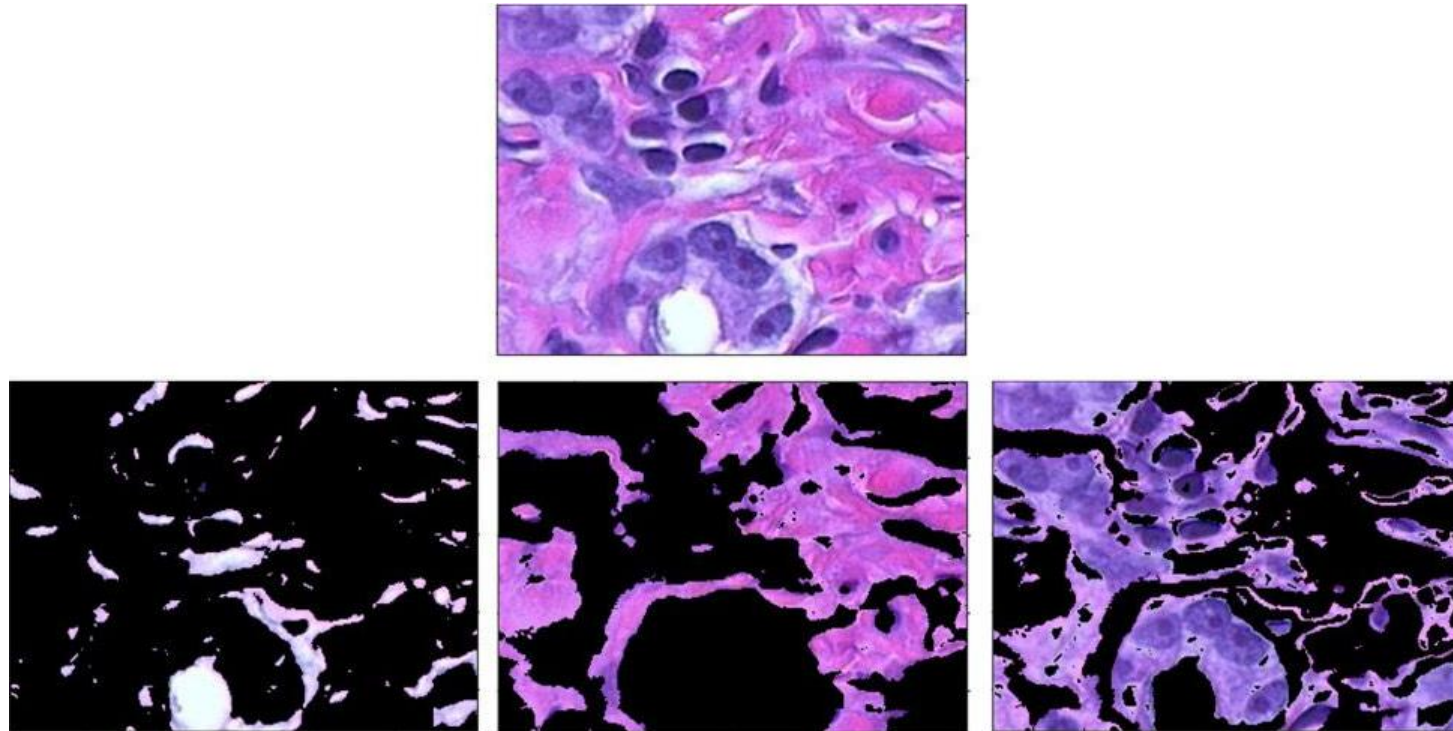
- Algorithms and techniques [\[https://www.mathworks.com/discovery/image-segmentation.html\]](https://www.mathworks.com/discovery/image-segmentation.html)
  - Developed over the years using domain-specific knowledge to effectively solve segmentation problems in specific application areas such as medical imaging, automated driving, video surveillance, and machine vision
  - Thresholding
    - Performs thresholding on a greyscale or color image to create a binary image





## – Clustering

- Creates a segmented labeled image using a specific clustering algorithm such as K-means clustering
- For example, to distinguish between tissue types in an image of body tissue stained with hematoxylin and eosin



## – Graph-based segmentation

- Enables to segment an image into foreground and background areas



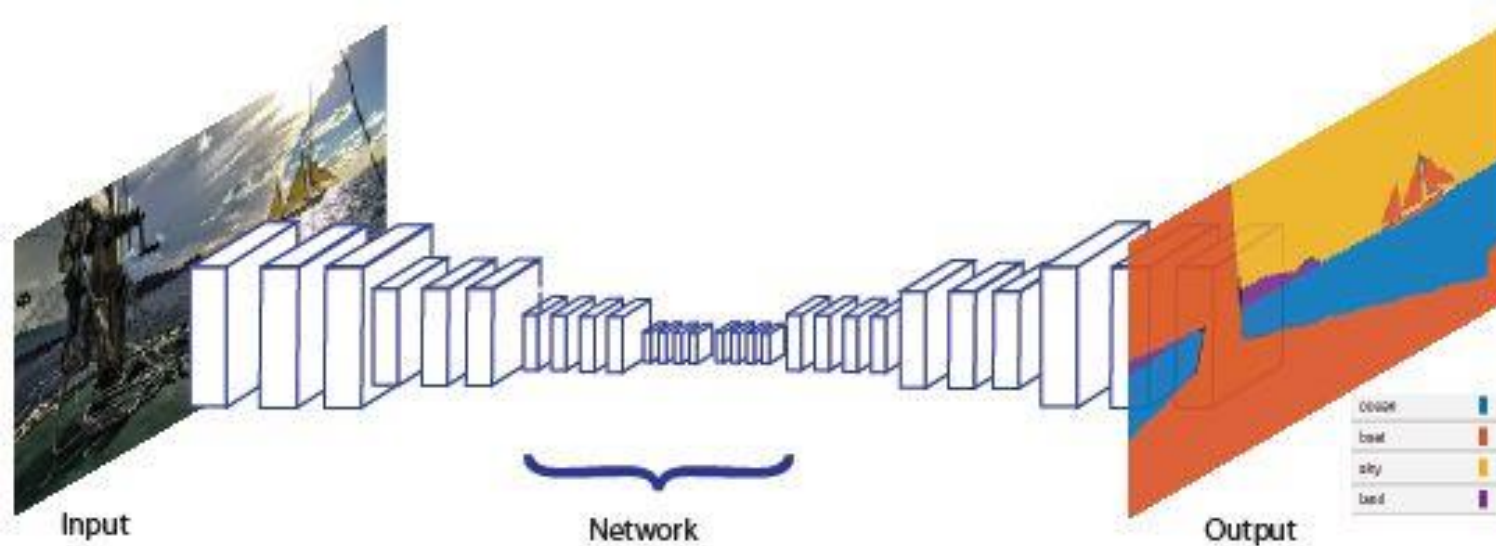
## – Region growing

- Examines neighbouring pixels of initial seed points and determines iteratively whether the pixel neighbours should be added to the area



# Deep Learning-based Image Segmentation

- Associates every pixel/voxel of an image with a class label by using neural networks



[<https://www.mathworks.com/discovery/image-segmentation.html>]

- Leverages the power of deep learning algorithms to analyze image features at various scales, offering improved accuracy and efficiency compared to traditional methods
- Processes the entire image in smaller sections vs. holistically
  - Patch-wise segmentation
    - Takes a small patch around a voxel as the input and traverses the entire volume by repeatedly taking patches
    - Redundant calculations caused by overlapping patches decreases computational efficiency
  - Semantic-wise segmentation
    - Takes the entire volume or a large patch as the input
    - Prone to overfitting during training due to class imbalance

- Segmentation performance

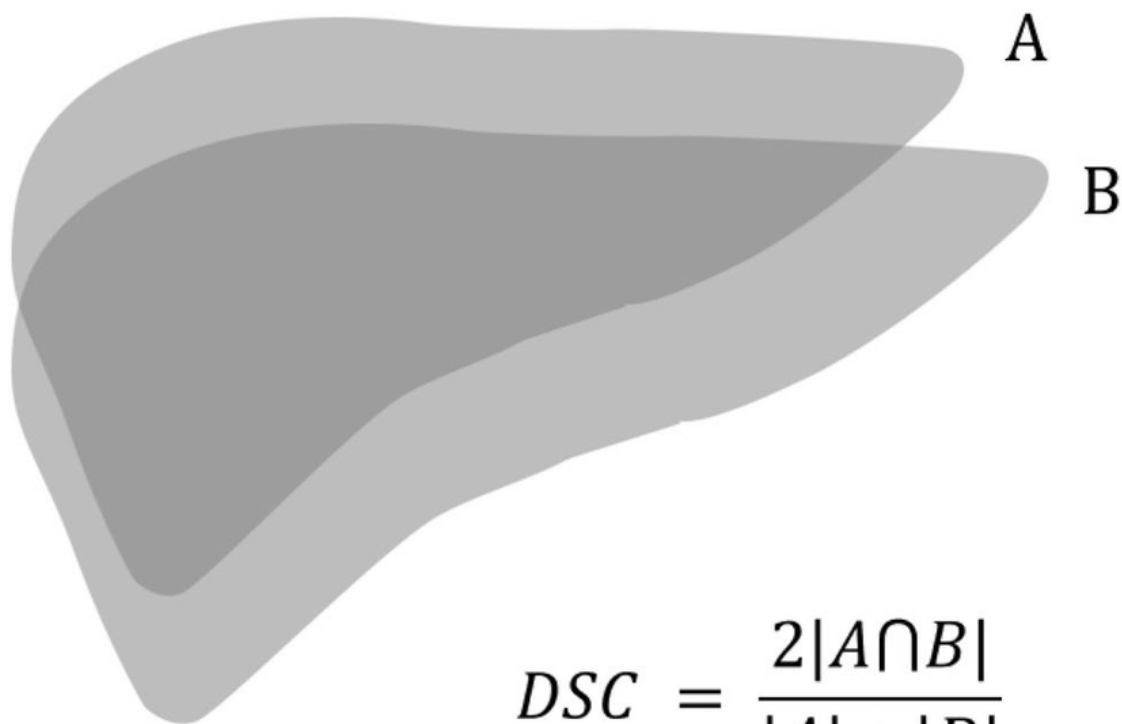
- Dice similarity coefficient (DSC, Dice-Sørensen coefficient or Dice coefficient) [\[Dice, 1945\]](#)

- $2 * |X \cap Y| / (|X| + |Y|)$ , where X and Y are the predicted and ground truth segmentations
    - Measures the overlap between predicted and ground truth segmentations
    - $F_1$  score that is a harmonic mean of precision and recall
      - Precision (True Positive Value (TPV)) =  $TP / (TP + FP)$
      - Recall (sensitivity) =  $TP / (TP + FN)$
      - $F_1$  score =  $2 / ((1 / \text{precision}) + (1 / \text{recall})) = 2TP / (2TP + FP + FN)$
    - Range: 0 (no overlap) to 1 (perfect overlap)
    - Sensitive to both false positives and false negatives

		Predicted condition			
		Positive (PP)	Negative (PN)	Informedness, bookmaker informedness (BM) $= \text{TPR} + \text{TNR} - 1$	Prevalence threshold (PT) $= \frac{\sqrt{\text{TPR} \times \text{FPR}} - \text{FPR}}{\text{TPR} - \text{FPR}}$
Actual condition	Positive (P)	True positive (TP), hit	False negative (FN), type II error, miss, underestimation	True positive rate (TPR), recall, sensitivity (SEN), probability of detection, hit rate, power $= \frac{\text{TP}}{\text{P}} = 1 - \text{FNR}$	False negative rate (FNR), miss rate $= \frac{\text{FN}}{\text{P}} = 1 - \text{TPR}$
	Negative (N)	False positive (FP), type I error, false alarm, overestimation	True negative (TN), correct rejection	False positive rate (FPR), probability of false alarm, fall-out $= \frac{\text{FP}}{\text{N}} = 1 - \text{TNR}$	True negative rate (TNR), specificity (SPC), selectivity $= \frac{\text{TN}}{\text{N}} = 1 - \text{FPR}$
	Prevalence $= \frac{\text{P}}{\text{P} + \text{N}}$	Positive predictive value (PPV), precision $= \frac{\text{TP}}{\text{PP}} = 1 - \text{FDR}$	False omission rate (FOR) $= \frac{\text{FN}}{\text{PN}} = 1 - \text{NPV}$	Positive likelihood ratio (LR+) $= \frac{\text{TPR}}{\text{FPR}}$	Negative likelihood ratio (LR-) $= \frac{\text{FNR}}{\text{TNR}}$
	Accuracy (ACC) $= \frac{\text{TP} + \text{TN}}{\text{P} + \text{N}}$	False discovery rate (FDR) $= \frac{\text{FP}}{\text{PP}} = 1 - \text{PPV}$	Negative predictive value (NPV) $= \frac{\text{TN}}{\text{PN}}$ $= 1 - \text{FOR}$	Markedness (MK), deltaP ( $\Delta p$ ) $= \text{PPV} + \text{NPV} - 1$	Diagnostic odds ratio (DOR) $= \frac{\text{LR}^+}{\text{LR}^-}$
	Balanced accuracy (BA) $= \frac{\text{TPR} + \text{TNR}}{2}$	<b>F<sub>1</sub> score</b> $= \frac{2\text{PPV} \times \text{TPR}}{\text{PPV} + \text{TPR}} = \frac{2\text{TP}}{2\text{TP} + \text{FP} + \text{FN}}$	Fowlkes–Mallows index (FM) $= \sqrt{\text{PPV} \times \text{TPR}}$	Matthews correlation coefficient (MCC) $= \frac{\sqrt{\text{TPR} \times \text{TNR} \times \text{PPV} \times \text{NPV}}}{\sqrt{\text{FNR} \times \text{FPR} \times \text{FOR} \times \text{FDR}}}$	Threat score (TS), critical success index (CSI), Jaccard index $= \frac{\text{TP}}{\text{TP} + \text{FN} + \text{FP}}$

[[https://en.wikipedia.org/wiki/Confusion\\_matrix](https://en.wikipedia.org/wiki/Confusion_matrix)]

## DSC or F<sub>1</sub> score in a confusion matrix



$$DSC = \frac{2|A \cap B|}{|A| + |B|}$$

DSC: Dice similarity coefficient



[Lee et al., 2018; <https://www.mathworks.com/help/images/ref/dice.html>]

## Computation of DSC

## – Intersection over Union (IoU, Jaccard Index)

- $|X \cap Y| / |X \cup Y|$
- Measures the overlap ratio of the intersection to the union of predicted and ground truth segmentations
- Range: 0 (no overlap) to 1 (perfect overlap)
- Stricter than DSC by penalizing errors more heavily

## – Mean Intersection over Union (mIoU)

- Average of IoU scores for all classes
- Provides an overall measure of segmentation quality across multiple classes
- Range: 0 (no overlap) to 1 (perfect overlap)
- Useful for multi-class segmentation tasks

## – Hausdorff distance

- $\max(h(X,Y), h(Y,X))$ , where  $h(X,Y) = \max(\min(d(x,y)))$  for  $x$  in  $X$ ,  $y$  in  $Y$  and  $h(Y,X) = \max(\min(d(y,x)))$  for  $y$  in  $Y$ ,  $x$  in  $X$
- Measures the maximum distance between the boundaries of predicted and ground truth segmentations
- Range: 0 to  $\infty$  (lower is better)
- Sensitive to outliers, useful for evaluating boundary accuracy

## – Average Surface Distance (ASD)

- Average of distances between surfaces of predicted and ground truth segmentations
- Measures the average error in boundary delineation
- 0 to  $\infty$  (lower is better)
- Less sensitive to outliers than Hausdorff Distance

## – Accuracy

- $(\text{Correctly Classified Pixels}) / (\text{Total Pixels}) = (TP + TN) / (\text{Total Pixels})$
- Measures the proportion of pixels correctly classified across all classes
- Range: 0 (completely incorrect classification) to 1 (perfect classification)

## – Sensitivity and specificity

- $\text{Sensitivity} = TP / (TP + FN)$ ,  $\text{specificity} = TN / (TN + FP)$
- Measure the model's ability to correctly identify positive and negative cases
- Range: 0 (complete failure to detect positive/negative cases) to 1 (perfect detection of positive/negative cases)

## – Area Under the Receiver Operating Characteristic Curve (AUC-ROC)

- Measures the model's ability to distinguish between classes
- Range: 0.5 (random guessing) to 1 (perfect classification)



- Deep learning-based lesion segmentation
  - Specific application of image segmentation to medical images by targeting abnormal tissues or pathological regions
  - Challenges
    - Class imbalance (lesions often small compared to healthy tissue)
    - Variabe in lesion shape, size, and location
    - Artifacts and noise common in medical images
  - Data considerations
    - Often works with 3D volumetric images (CT, MRI scans)
    - Requires expert annotations, which can be costly and time-consuming
    - Employs data augmentation to efficiently use limited training data
    - May benefit from multi-modal data integration

## – Performance metrics

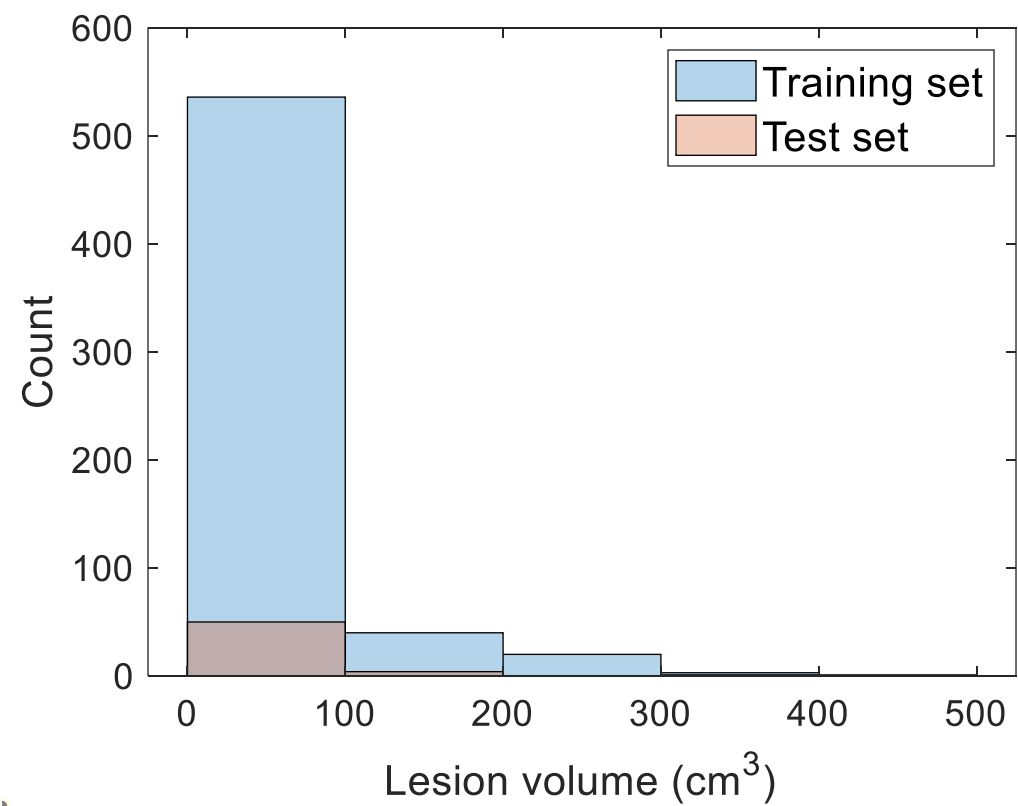
- Usually uses domain-specific metrics like DSC and Hausdorff distance
- Emphasizes both quantitative accuracy and clinical relevance

## – Specialized architectures

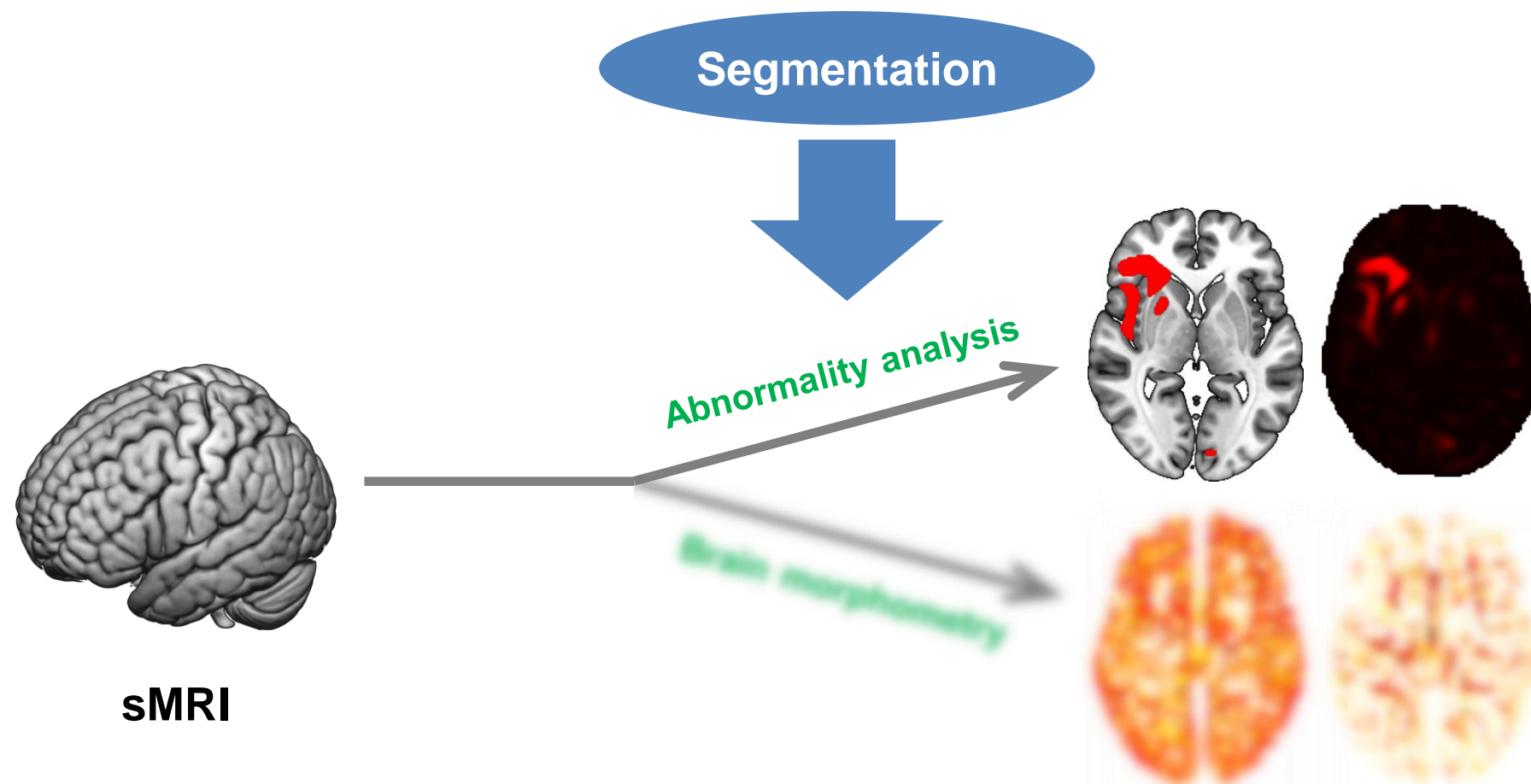
- Uses common segmentation models such as U-Net and its variants
  - Ability to capture both local and global context
  - Skip connections that preserve fine details, crucial for precise lesion boundaries
- Designed to handle medical imaging specificities

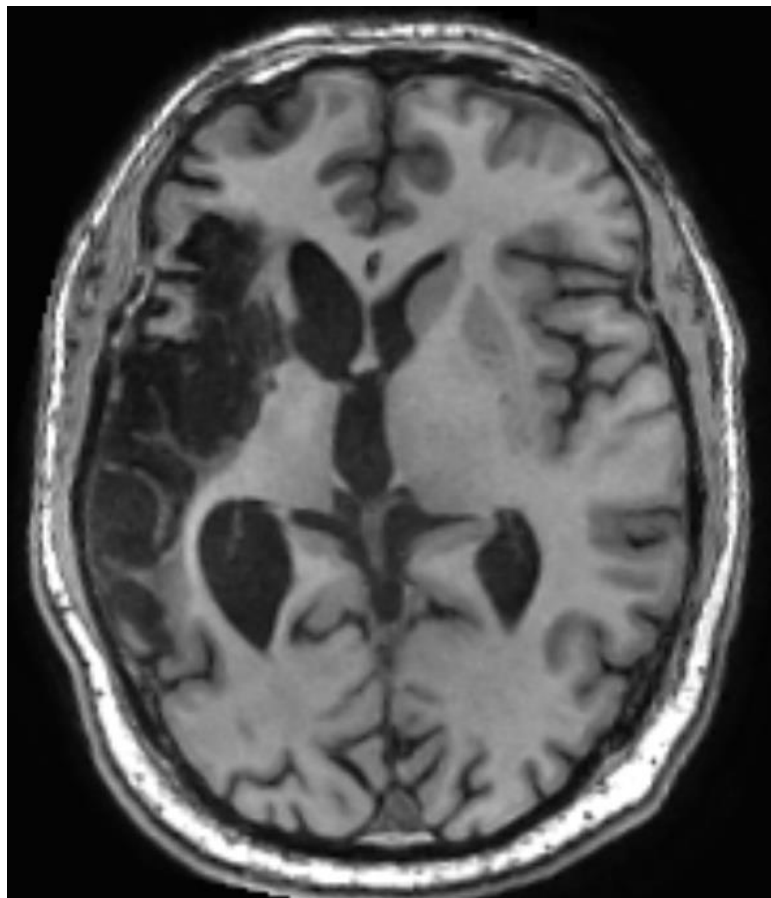
# Dataset

- ATLAS v2.0 dataset for training ( $n = 655$ )
  - Training set:  $n = 600$ 
    - T1-weighted MRI scans: [train/Brain/001-600.nii.gz](#)
    - Lesion masks: [train/Lesion/001-600.nii.gz](#)
  - Test set:  $n = 55$ 
    - T1-weighted MRI scans: [test/Brain/001-055.nii.gz](#)
    - Lesion masks: hidden



**Distribution of lesion volume**

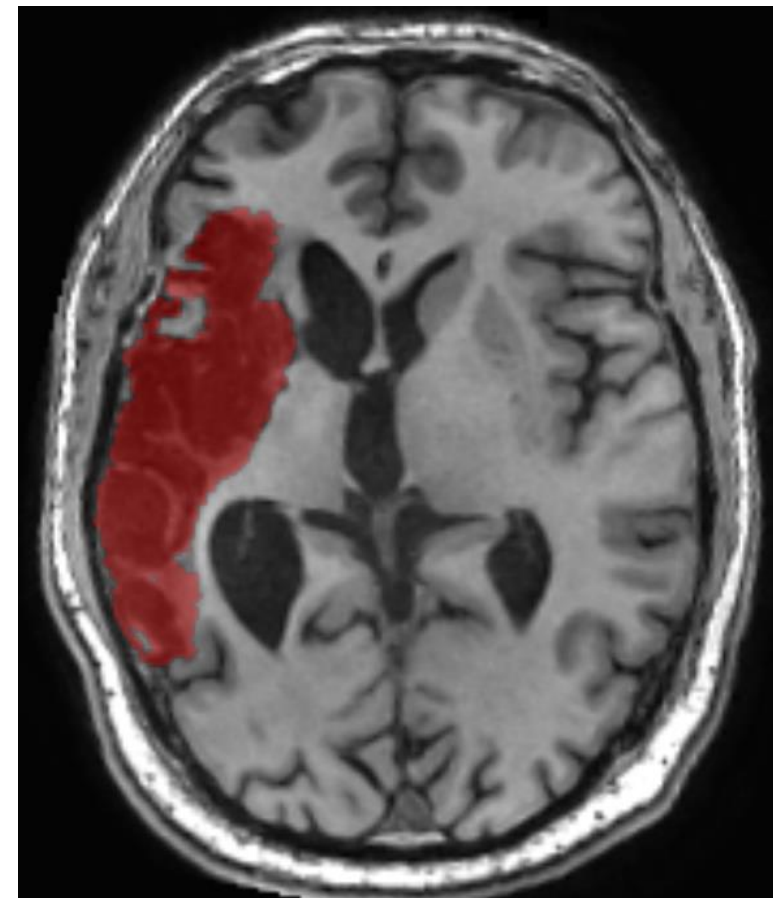




Brain



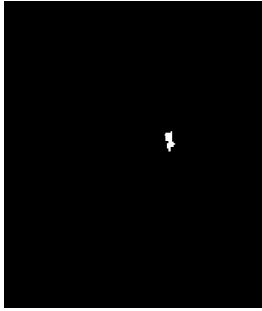
Lesion



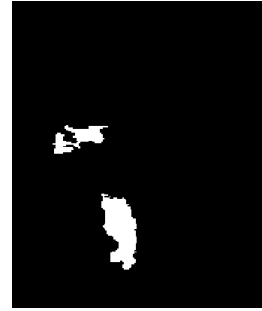
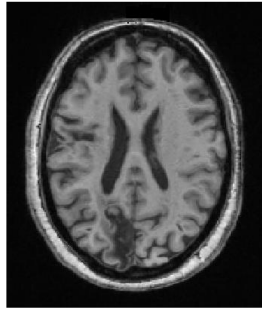
Lesion-overlaid brain

**Example pair of a T1-weighted MRI scan and a lesion mask**

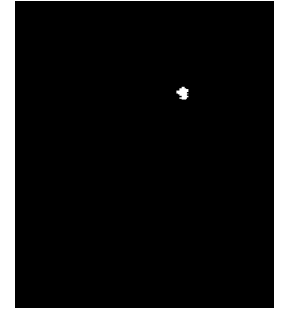
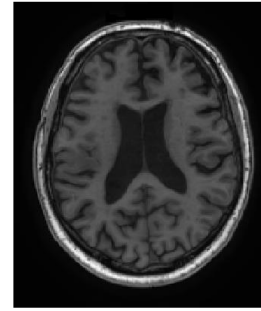
001: 0.884 cm<sup>3</sup>



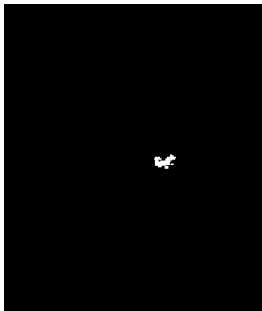
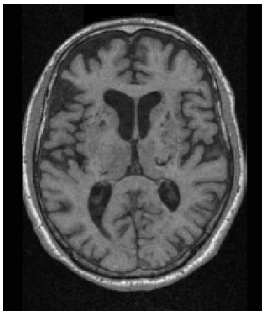
002: 33.781 cm<sup>3</sup>



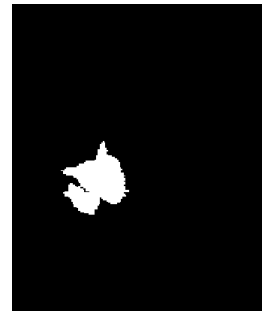
003: 0.351 cm<sup>3</sup>



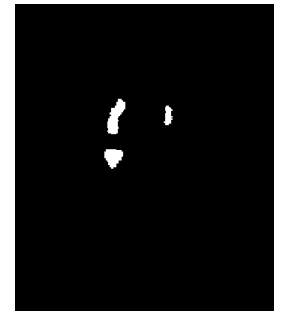
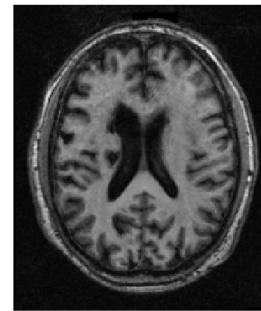
004: 1.417 cm<sup>3</sup>



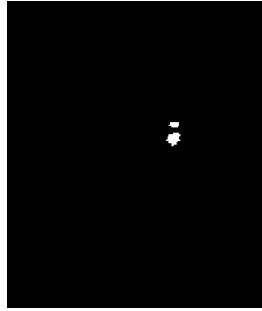
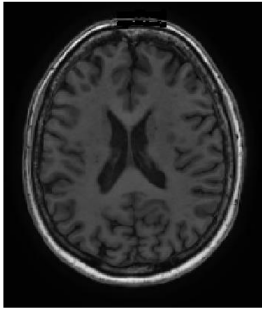
005: 62.252 cm<sup>3</sup>



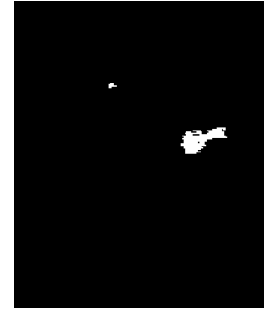
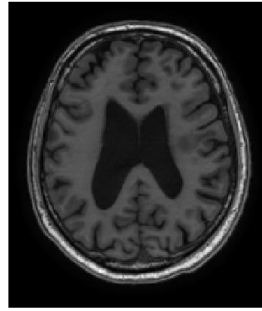
006: 7.201 cm<sup>3</sup>



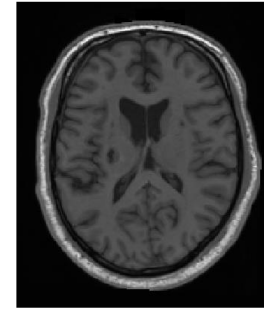
007: 1.426 cm<sup>3</sup>



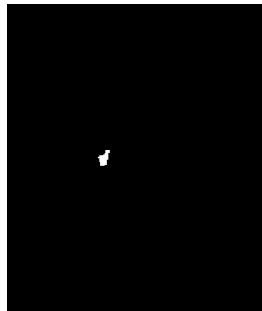
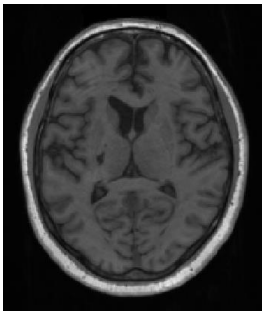
008: 16.002 cm<sup>3</sup>



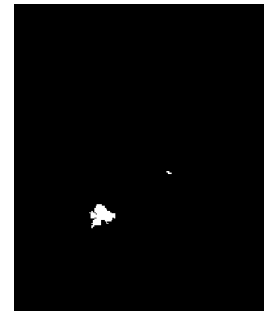
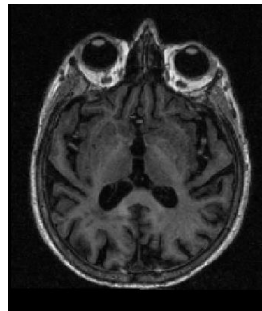
009: 2.852 cm<sup>3</sup>



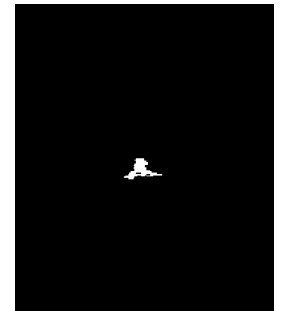
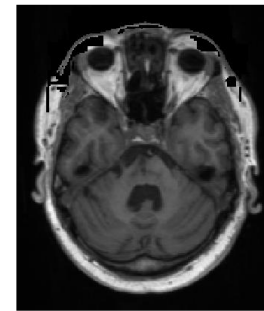
010: 0.509 cm<sup>3</sup>



011: 3.549 cm<sup>3</sup>

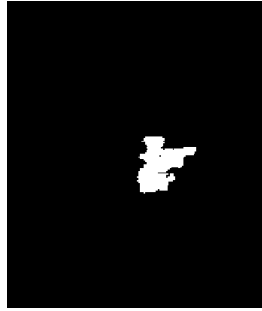
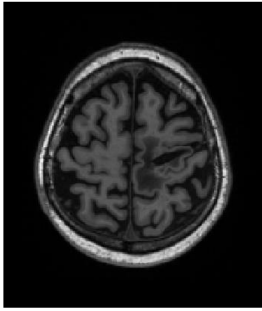


012: 1.024 cm<sup>3</sup>

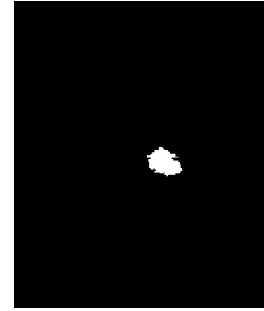
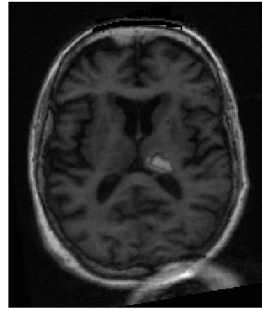




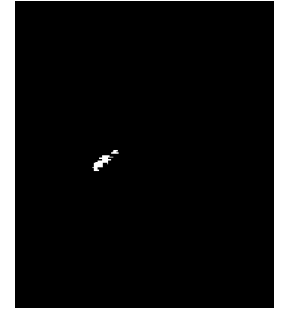
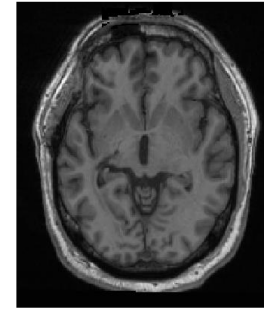
013: 48.023 cm<sup>3</sup>



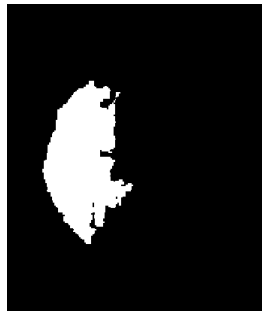
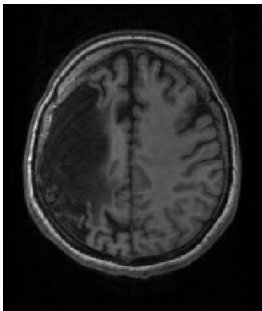
014: 6.257 cm<sup>3</sup>



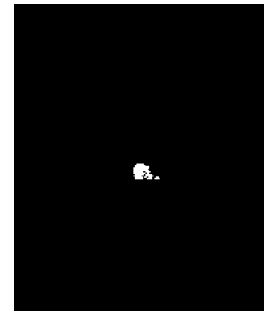
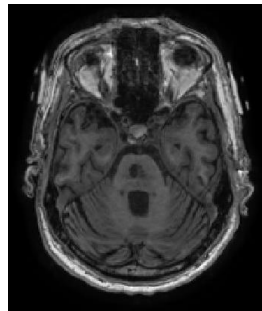
015: 1.637 cm<sup>3</sup>



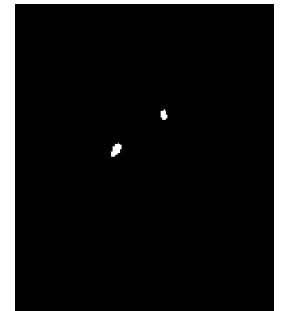
016: 396.194 cm<sup>3</sup>



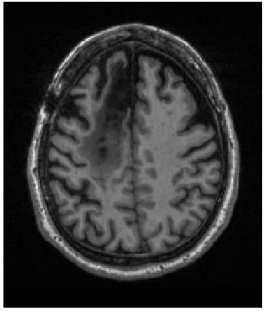
017: 2.487 cm<sup>3</sup>



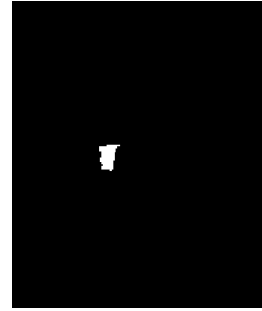
018: 0.689 cm<sup>3</sup>



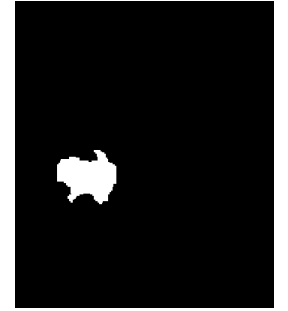
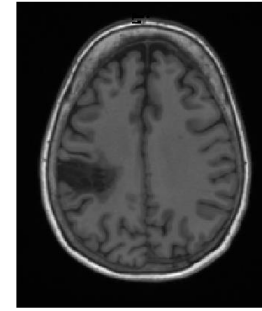
019: 110.638 cm<sup>3</sup>



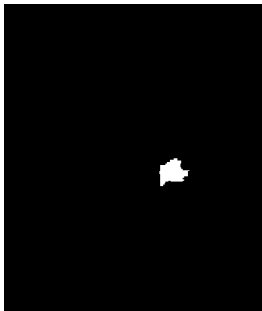
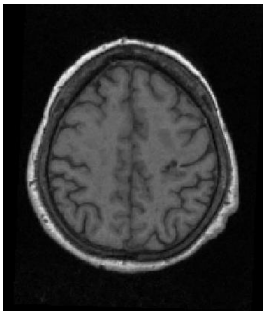
020: 2.196 cm<sup>3</sup>



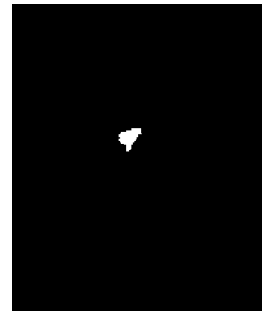
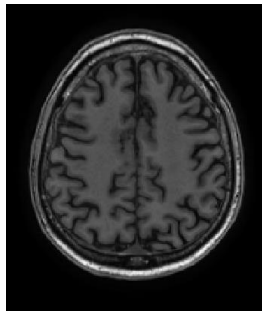
021: 30.117 cm<sup>3</sup>



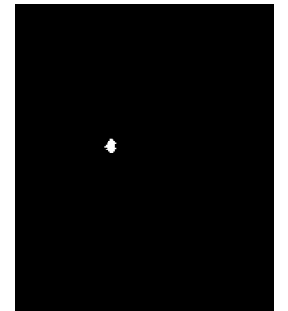
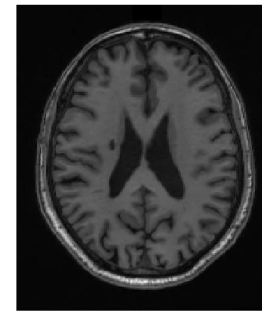
022: 4.550 cm<sup>3</sup>



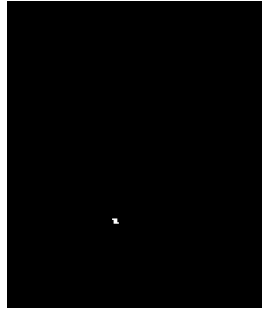
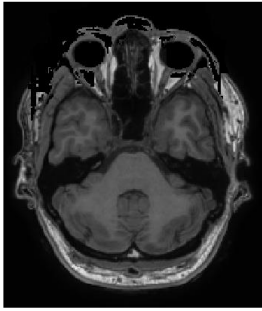
023: 1.812 cm<sup>3</sup>



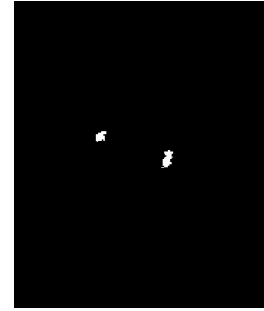
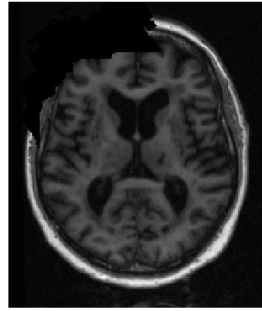
024: 1.220 cm<sup>3</sup>



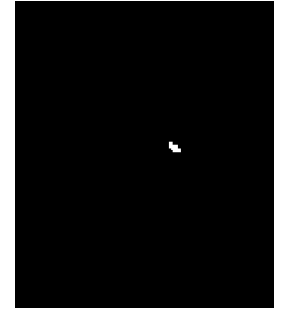
025: 0.043 cm<sup>3</sup>



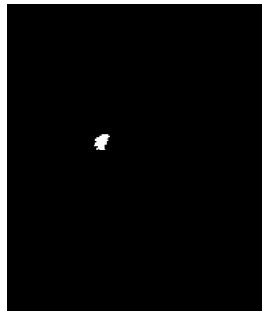
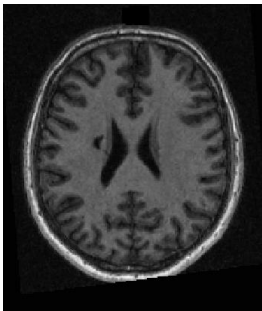
026: 1.910 cm<sup>3</sup>



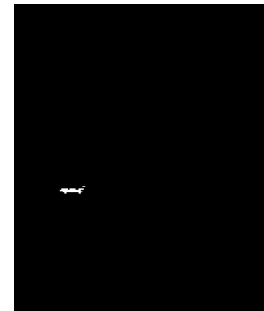
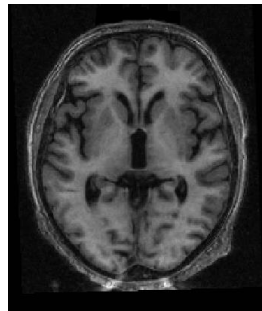
027: 0.433 cm<sup>3</sup>



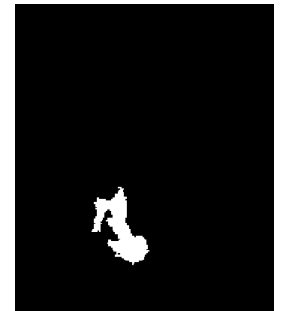
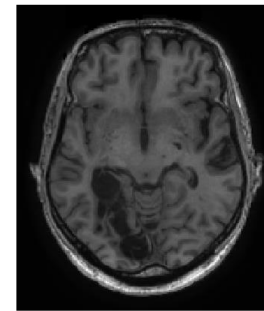
028: 1.143 cm<sup>3</sup>



029: 0.483 cm<sup>3</sup>



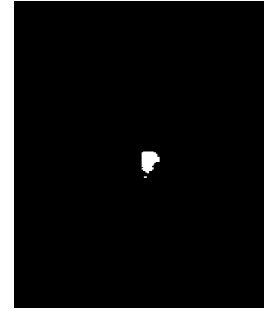
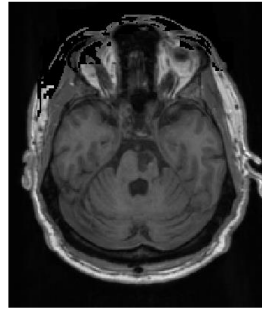
030: 12.176 cm<sup>3</sup>



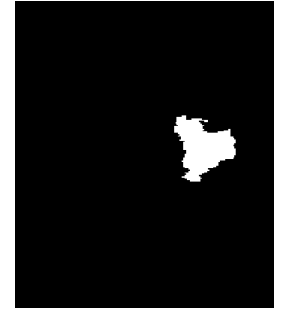
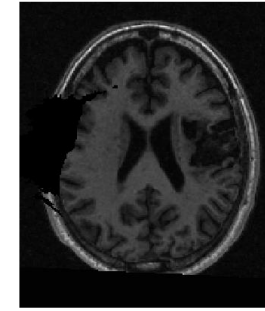
031: 33.231 cm<sup>3</sup>



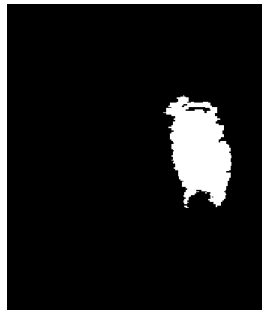
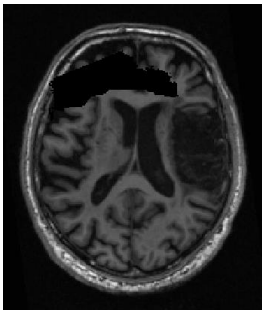
032: 1.776 cm<sup>3</sup>



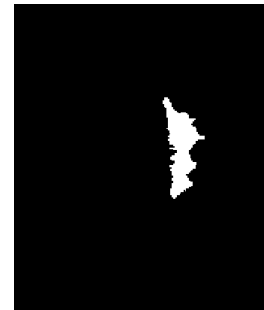
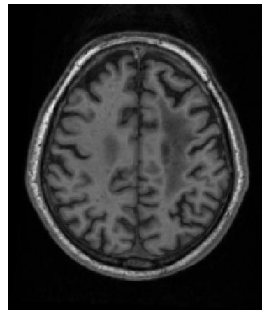
033: 41.860 cm<sup>3</sup>



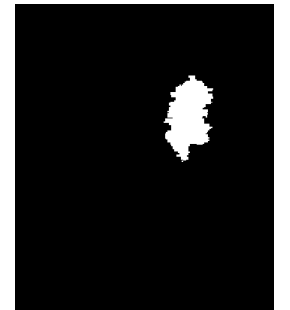
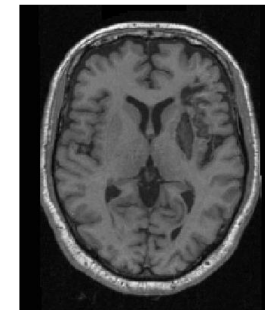
034: 102.925 cm<sup>3</sup>



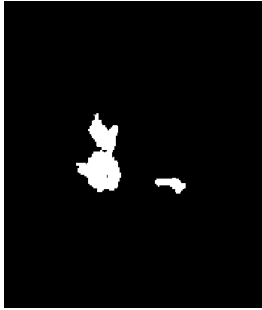
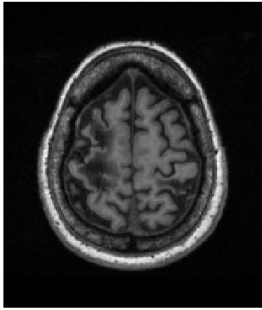
035: 47.787 cm<sup>3</sup>



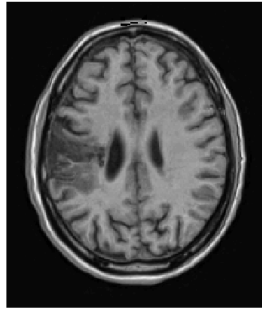
036: 72.786 cm<sup>3</sup>



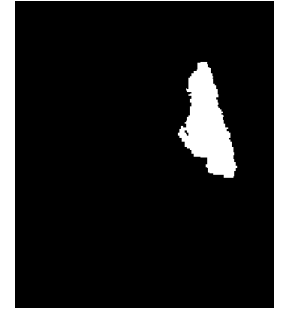
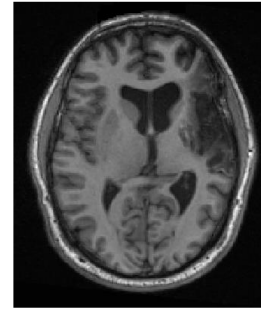
037: 36.236 cm<sup>3</sup>



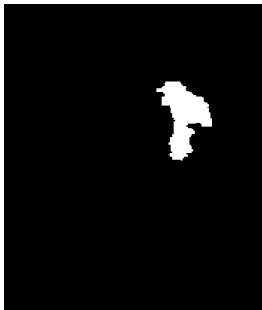
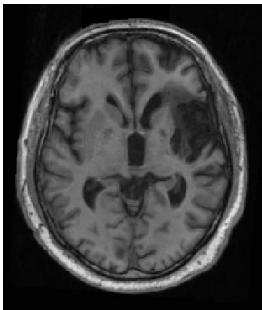
038: 67.076 cm<sup>3</sup>



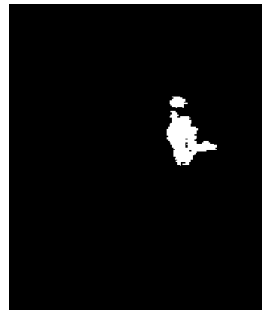
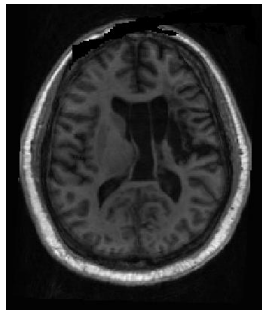
039: 140.210 cm<sup>3</sup>



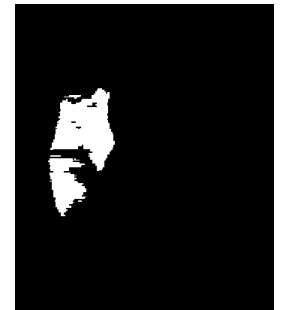
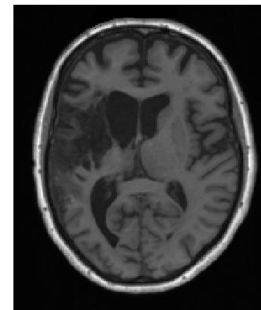
040: 53.083 cm<sup>3</sup>



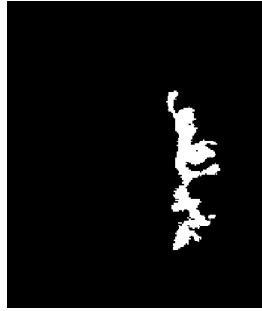
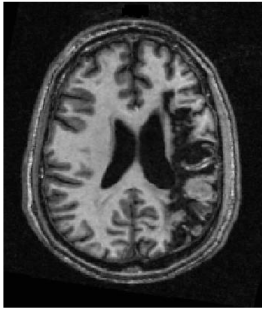
041: 24.708 cm<sup>3</sup>



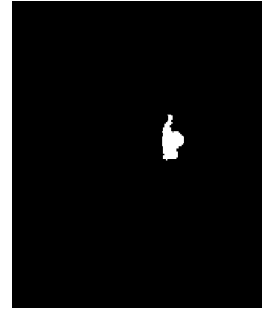
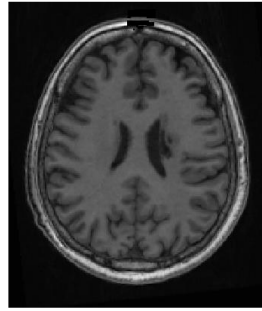
042: 119.731 cm<sup>3</sup>



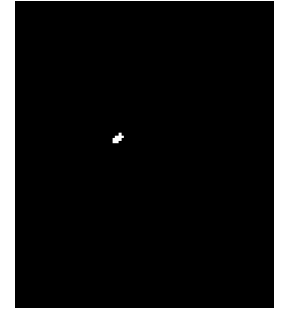
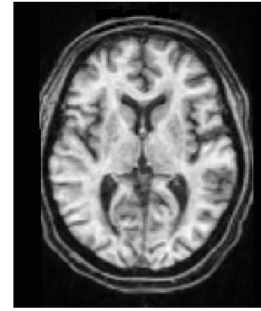
043: 86.768 cm<sup>3</sup>



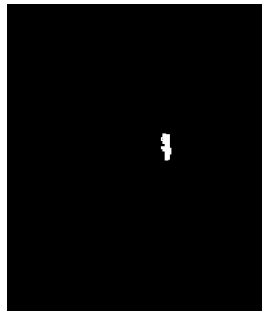
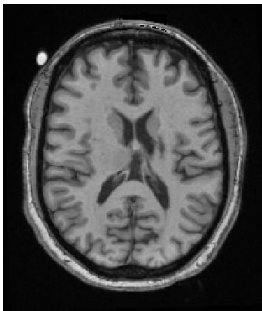
044: 4.925 cm<sup>3</sup>



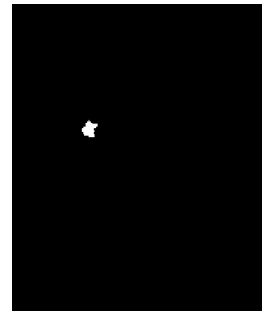
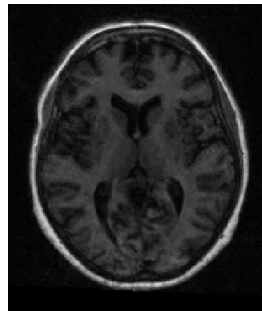
045: 0.352 cm<sup>3</sup>



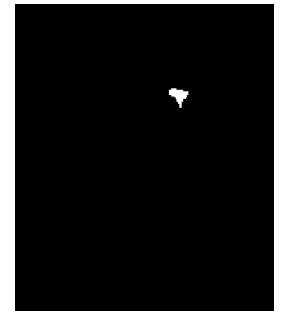
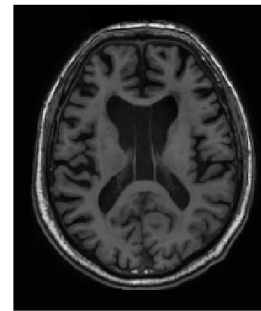
046: 0.528 cm<sup>3</sup>



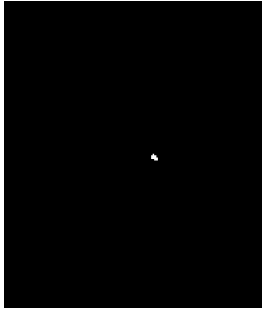
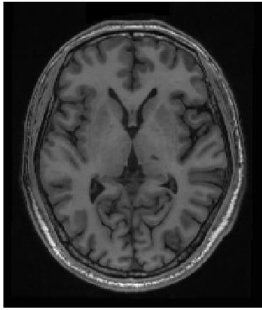
047: 0.582 cm<sup>3</sup>



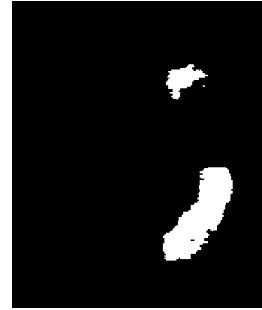
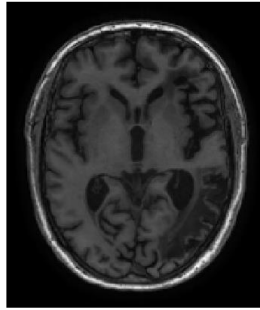
048: 3.009 cm<sup>3</sup>



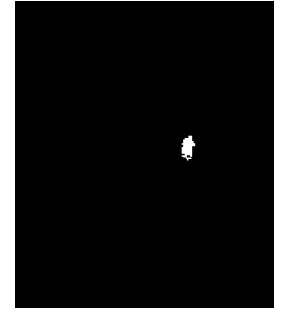
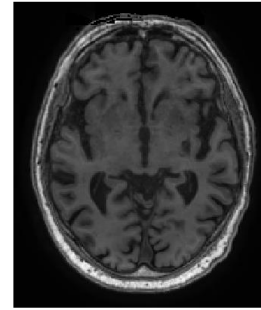
049: 0.069 cm<sup>3</sup>



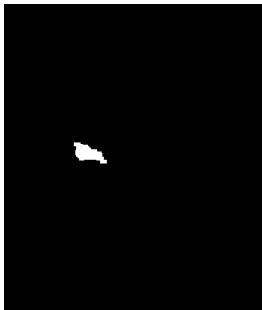
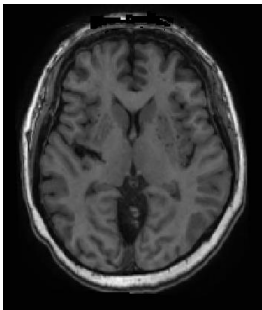
050: 88.918 cm<sup>3</sup>



051: 2.994 cm<sup>3</sup>



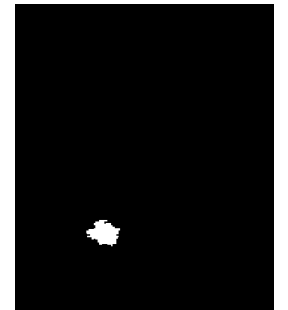
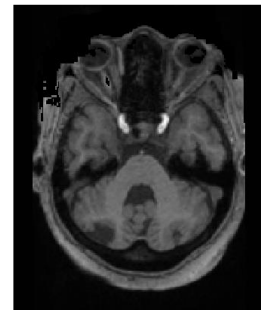
052: 3.191 cm<sup>3</sup>



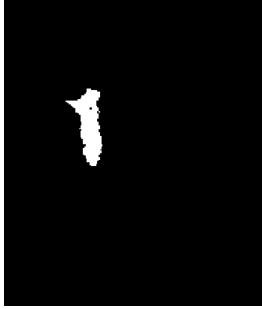
053: 8.246 cm<sup>3</sup>



054: 5.758 cm<sup>3</sup>



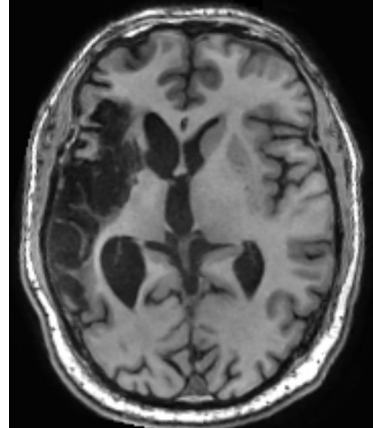
055: 26.097 cm<sup>3</sup>





- T1-weighted MRI scan and lesion mask
  - T1-weighted MRI scan in the native brain space
  - Lesion mask in the native brain space

T1-weighted MRI scan



Lesion mask



**1 mm:**

**Dimensions:**  $197 \times 233 \times 189$

**Voxel size:**  $1.0 \text{ mm} \times 1.0 \text{ mm} \times 1.0 \text{ mm}$

**2 mm:**

**Dimensions:**  $98 \times 116 \times 94$

**Voxel size:**  $2.0 \text{ mm} \times 2.0 \text{ mm} \times 2.0 \text{ mm}$

**T1-weighted MRI scan and lesion mask**

- Segmentation label map
  - Lesion mask
- Lesion segmentation performance
  - Mean DSC for the test set ( $n = 55$ )
    - Average of the overlap between predicted and manually annotated lesion masks across the test set
    - Ranges from 0 to 1

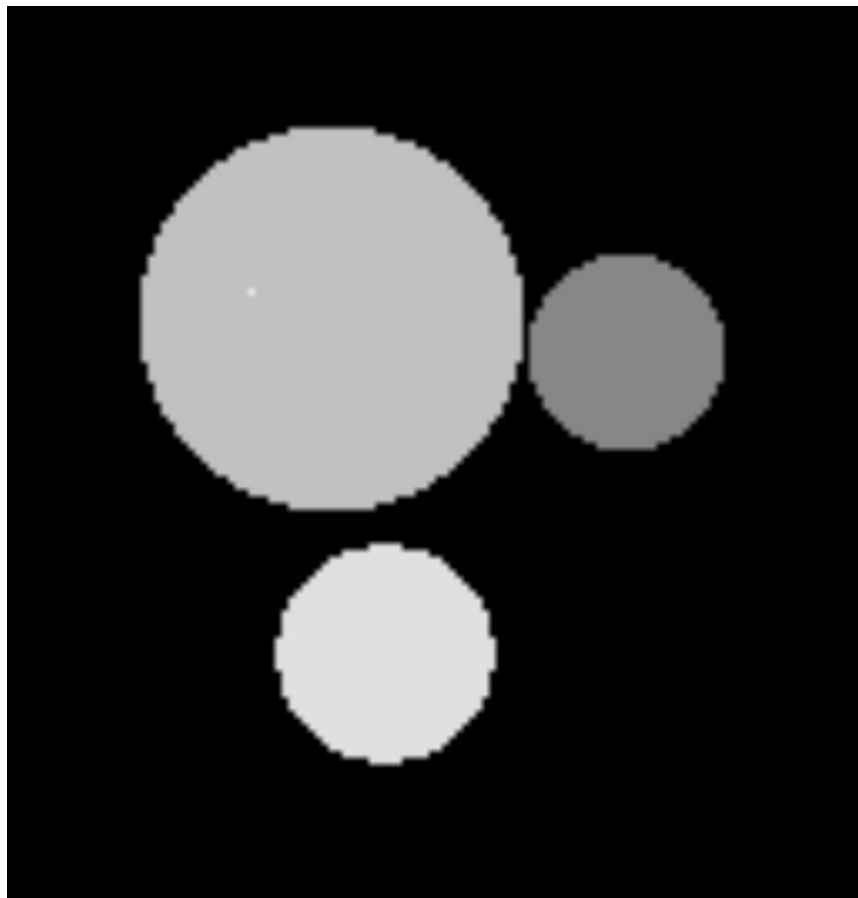
Article	Method	Reported Dice	Code Publicly Available	<i>n</i>	Validation Method	Input size 2D/3D (H, W, D)
					<b>Cross-validation</b>	
Basak <i>et al.</i> , 2021	DFENet	0.546	no	229	5-fold cross-validation	2D 192, 192 or 3D 192, 192, 4
Hui <i>et al.</i> , 2020	PSPF and U-Net	0.593	no	239	6-fold cross-validation	2D 176, 176
Lu <i>et al.</i> , 2020	EDCL w/ 3D Unet	0.148 (0.584)**	no	239	5-fold cross-validation	3D 64, 64, 64
Qi <i>et al.</i> , 2019	X-Net	0.487	yes	229	5-fold cross-validation	2D 192, 224
Zhang <i>et al.</i> , 2020	MI-UNet	0.567	no	229	5-fold cross-validation	2D 233, 197 or 3D 49, 49, 49
					<b>One hold-out Train, Validation, Test</b>	
Chen <i>et al.</i> , 2018	U-Net/GMM*	0.500/0.170	no	220	unclear/0, 0, 100 (%)	2D 128, 128 or 256, 256
Chen <i>et al.</i> , 2020	VAE*/GMVAE*	0.110/0.120	no	220	0, 0, 100/0, 0, 100 (%)	2D 200, 200
Kervadec <i>et al.</i> , 2020	Enet	0.474	yes	229	203, 26, 0	unclear
Liu <i>et al.</i> , 2019	MSDF-Net	0.558	no	229	160, 69, 0	2D 224, 177
Paing <i>et al.</i> , 2021	3D U-Net	0.668	no	239	60, 20, 20 (%)	3D 197, 233, 189
Qi <i>et al.</i> , 2020	U-Net	0.518	no	229	120, 40, 69	2D 224, 192
Sahayam <i>et al.</i> , 2020	MUDCap3	0.670	no	229	160, 69, 0	3D 256, 256, 256
Tomita <i>et al.</i> , 2020	3D-ResU-Net	0.640	yes	239	76, 11, 13 (%)	3D 144, 172, 168
Wang <i>et al.</i> , 2020	CPGAN	0.617	no	239	129, 40, 60	2D 256, 256
Xue <i>et al.</i> , 2020	U-Net (9 paths)	0.540	yes	54	0, 0, 54	3D 192, 224, 192
Yang <i>et al.</i> , 2019	CLCI-Net	0.581	yes	220	55, 18, 27 (%)	2D 224–233, 176–197
Zhou <i>et al.</i> , 2019	D-Unet	0.535	no	229	80, 20, 0 (%)	2D 192, 192 or 3D 192, 192, 4

[Liew et al., 2022]

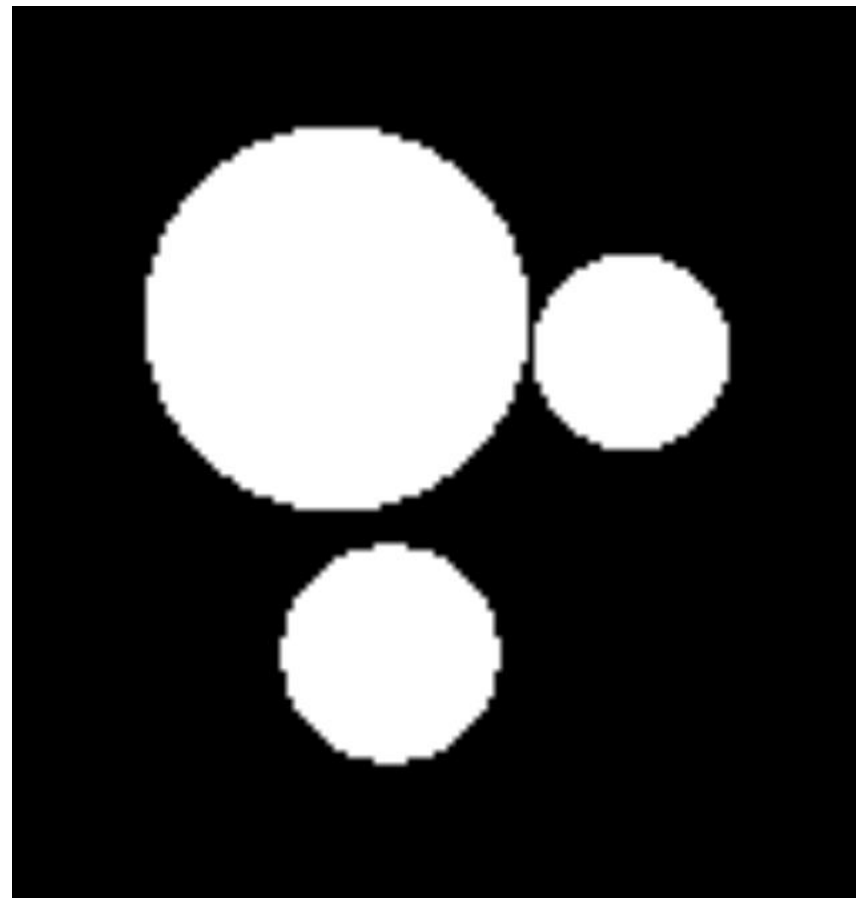
## Performance of lesion segmentation using ATLAS v1.2

# Demo Dataset

- Simulated images and labels
  - Training dataset:  $n = 40$ 
    - Images: [Image/0-39.nii.gz](#)
    - Masks: [Label/0-39.nii.gz](#)



Image



Label

**Example pair of an image and a label mask**