

Hypothesis-driven dimension reduction & source separation for time-domain EEG data

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Slides & code: git.io/JUPXf

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Outline

Symposium - To predict or not to predict: Modeling EEG data, promises, and limitations

What are and why use multivariate methods?

Generalized eigendecomposition (GED)

Using simulations to understand and implement GED

Empirical results

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3 Multivariate methods

What & why?

Cohen (2017, J Neuro Methods)
Cohen (2017, Trends in Neurosciences)
Grootswager et al. (2017, J Cog Neuro)

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Multivariate methods leverage EEG data's rich spatiotemporal structure

ERPs highlight event-related activity and ↑ signal-to-noise ratio

- *information is lost during averaging*

Univariate methods (ERPs) analyze individual electrodes separately

- *neurocognitive processes are encoded in spatiotemporal patterns*

Volume conduction: neural sources are mixed at the electrodes

- *ERPs don't unmix overlapping spatial and temporal information*

Multivariate methods address these problems!

4 How to implement GED

Generalized eigendecomposition (GED) framework

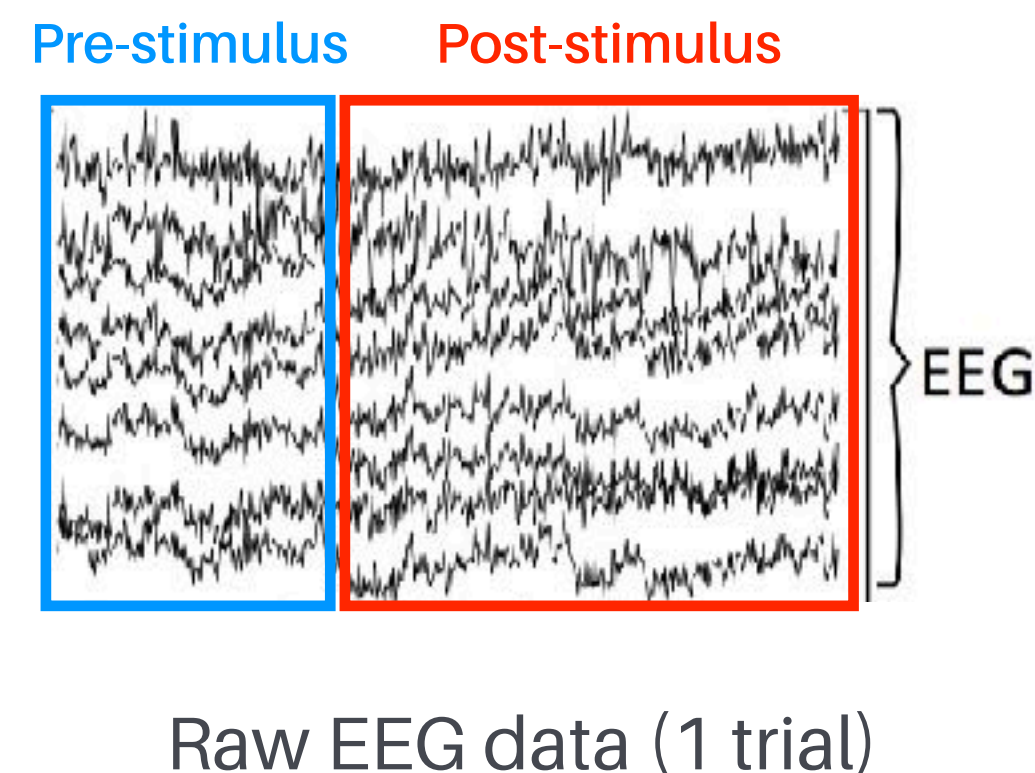
Cohen (2017, eLife)
Cohen (2017, J Neuro Methods)
Parra & Sajda (2003, J Mach Learn Res)
Parra et al. (2005, NeuroImage)

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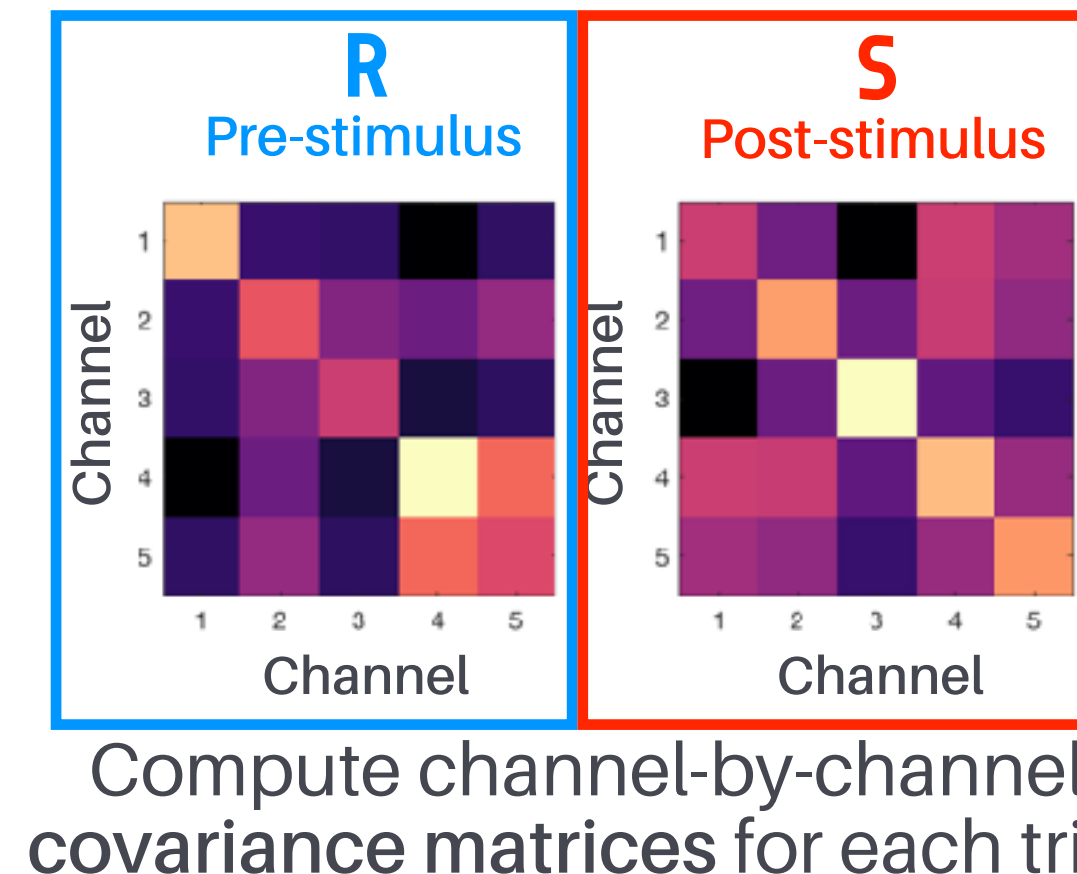
Ideal (and designed) for testing hypotheses

Directly contrasts two “conditions”

- hypothesis-driven (not “blind” source separation)
- represented by covariance matrices **R** and **S** (reference, signal)



```
% dat: trial 1 chan-by-time matrix
dat = EEG.data(:, :, 1);
% remove third dimension
dat = squeeze(dat);
```



```
% datR: select first 100 timepoints (pre-stimulus)
datR = dat(:, 1:100);
R = cov(datR');
% datS: select remainder timepoints (post-stimulus)
datS = dat(:, 101:end);
S = cov(datS');
```

Multivariate:
Considers
relationships/
between
channels

Compute **R** and **S** covariance matrices separately for each trial

```
% MATLAB implementation (assumes EEG variable is EEGLAB's EEG structure)
```

```
% STEP 1: initialize empty covariance matrices (chan-by-chan covariance matrix)
```

```
[R, S] = deal(zeros(EEG.nbchan)); % R (reference), S (signal)
```

```
% STEP 2: compute covariance R, S matrices for each trial
```

```
for ti=1:EEG.trials % for each trial
```

```
    datR = squeeze(EEG.data(:,1:100,ti)); % get pre-stimulus data
```

```
    R = R + cov(datR'); % compute covariance matrix R and sum them
```

```
    datS = squeeze(EEG.data(:,101:end,ti)); % get post-stimulus data
```

```
    S = S + cov(datS'); % compute covariance matrix S and sum them
```

```
end
```

```
% STEP 3: compute average covariance (divide by total number of trials)
```

```
R = R./EEG.trials;
```

```
S = S./EEG.trials;
```

6 How to implement GED

Generalized eigendecomposition (GED) framework

Cohen (2017, eLife)
Cohen (2017, J Neuro Methods)
Parra & Sajda (2003, J Mach Learn Res)
Parra et al. (2005, NeuroImage)

Conceptually simple and computationally efficient

Similar to principal component analysis (PCA)

- PCA: simplified, special case of GED
 - solves the basic eigenvalue equation: $\mathbf{S}\mathbf{w} = \mathbf{w}\lambda$
 - `[evecs, evals] = eig(S);`
- GED generalizes equation to two matrices: $\mathbf{S}\mathbf{w} = \mathbf{R}\mathbf{w}\lambda$
 - `[evecs, evals] = eig(S, R);`

7 How to implement GED

Generalized eigendecomposition (GED) framework

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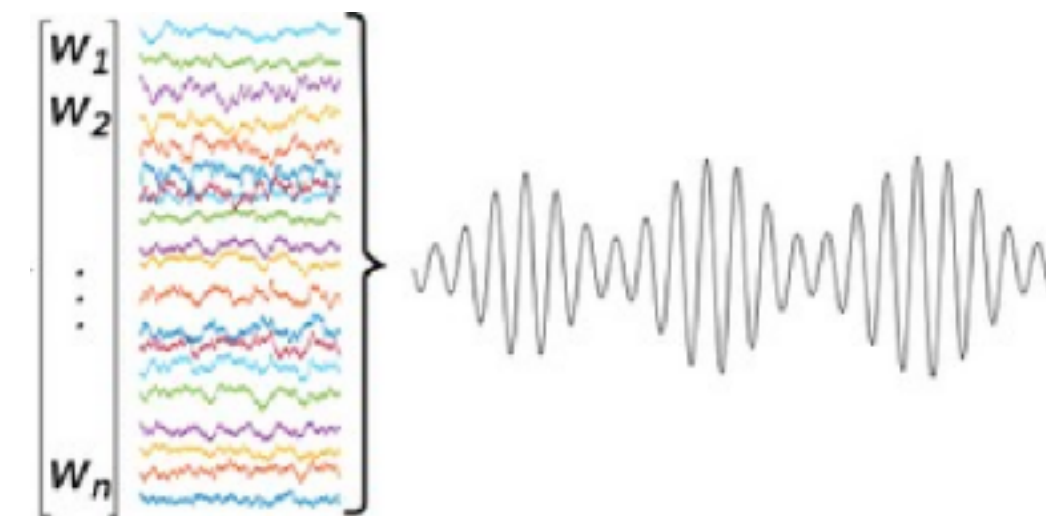
Reduces data dimensions and separates sources

Eigenvectors (`evecs`): spatial filters for computing components

Eigenvalues (`evals`): importance of components

Eigenvectors/components are **independent** but **not orthogonal**

- PCA doesn't separate sources well because sources are orthogonal



Apply weights/filters to original data to unmix sources

```
% topography for sources/components 1 & 2
topography_component1 = evecs(:,1)*S;
topography_component2 = evecs(:,2)*S;

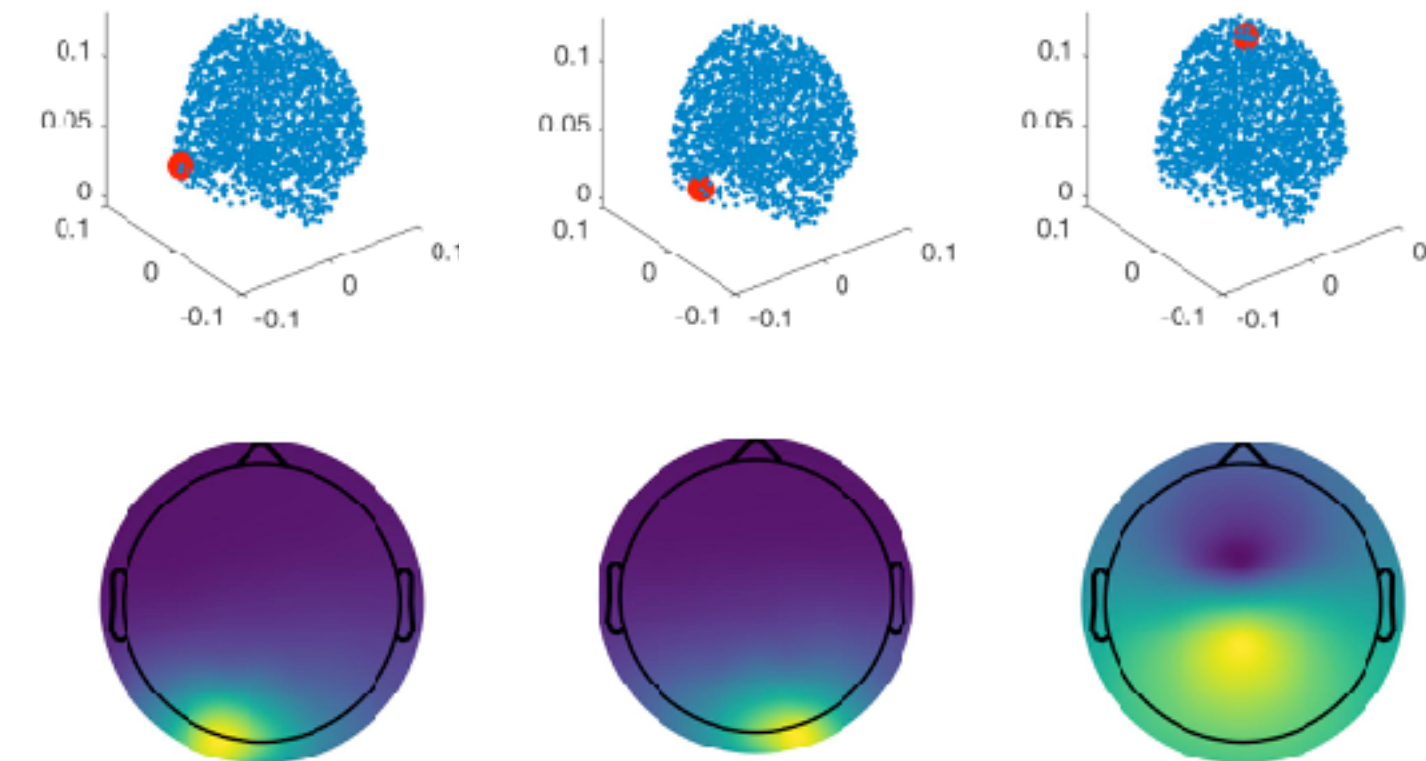
% time series for sources/components 1 & 2
comp_ts = evecs(:,1:2)'*reshape(EEG.data,EEG.nbchan,[]);
comp_ts = reshape(comp_ts,[2 EEG.pnts EEG.trials]);
```

8 Simulation

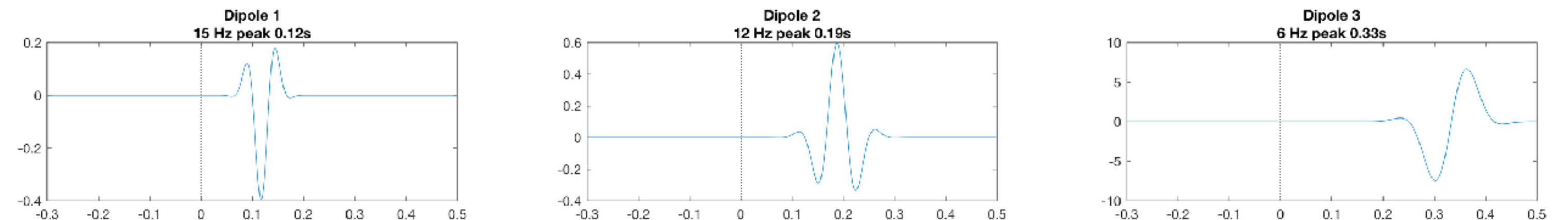
Defining simulation parameters

Lin & Cohen (in prep)

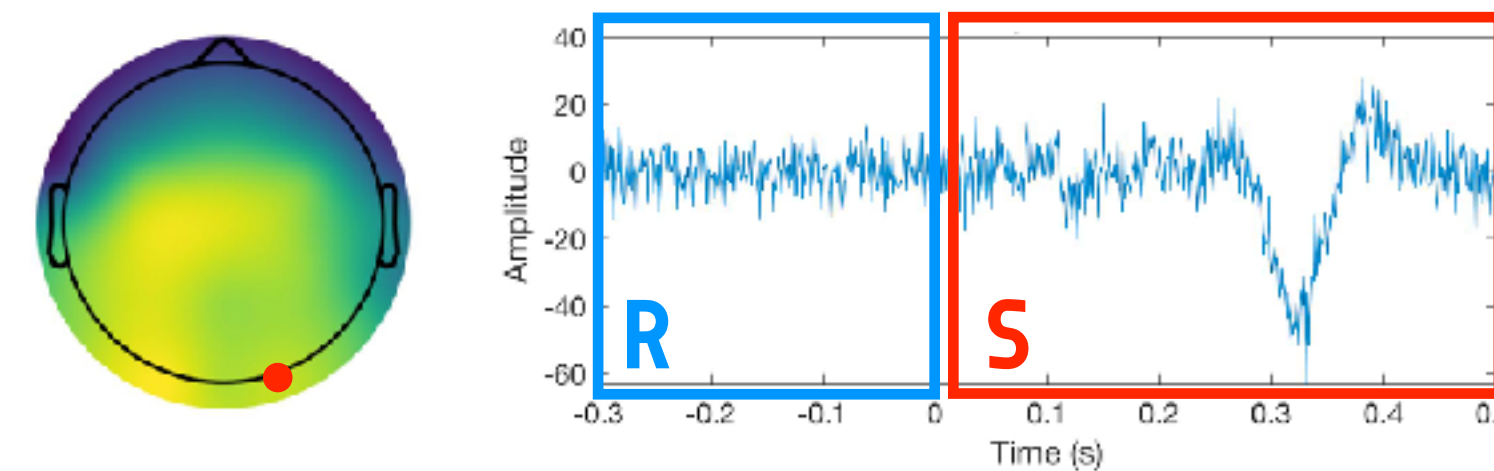
Spatial locations and topographies of 3 dipole sources



Simulated pure neural signals



Mixing of neural signals and noise + projection to the scalp



"Observed" topography and ERP

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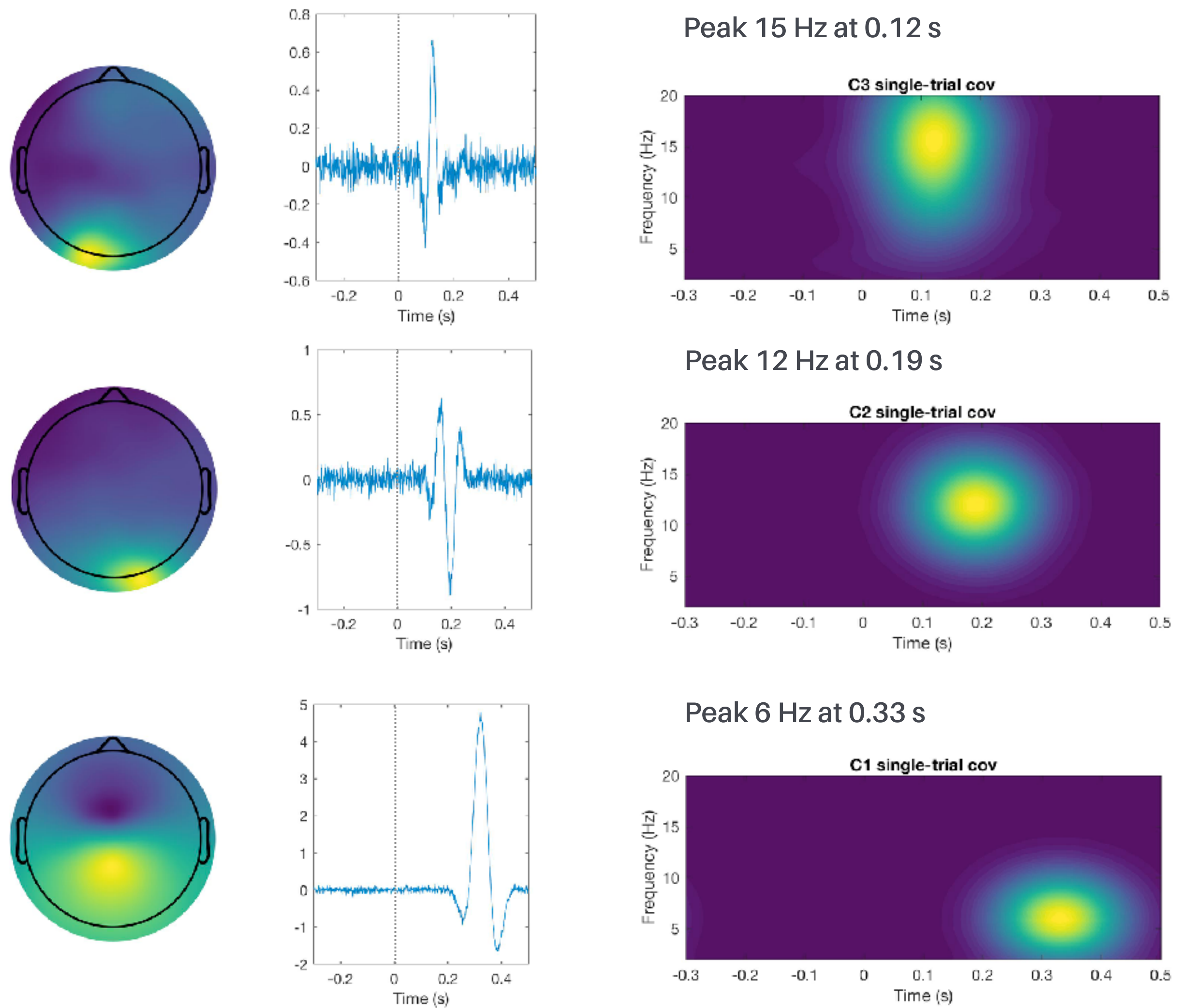
9 Parameter recovery

Recovering parameters from noisy simulated data

Lin & Cohen (in prep)

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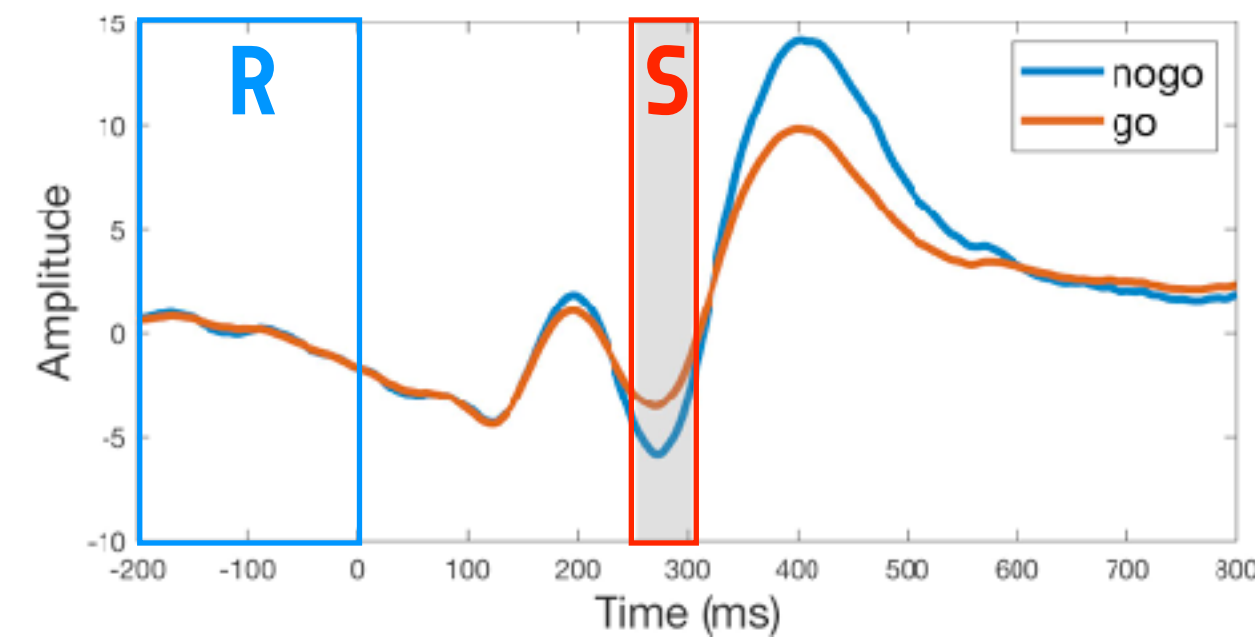
GED recovers simulated spatiotemporal and spectral dynamics



Conflict-monitoring

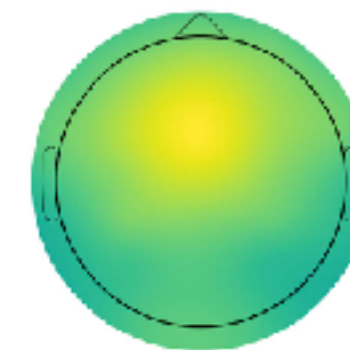
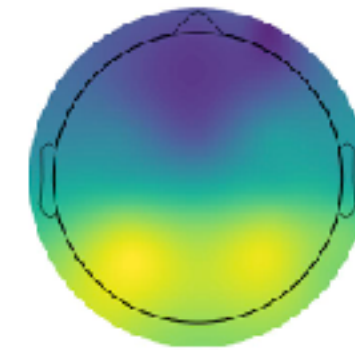
Lin & Cohen (in prep)

Go/no-go task N2 ERP (254 to 304 ms)

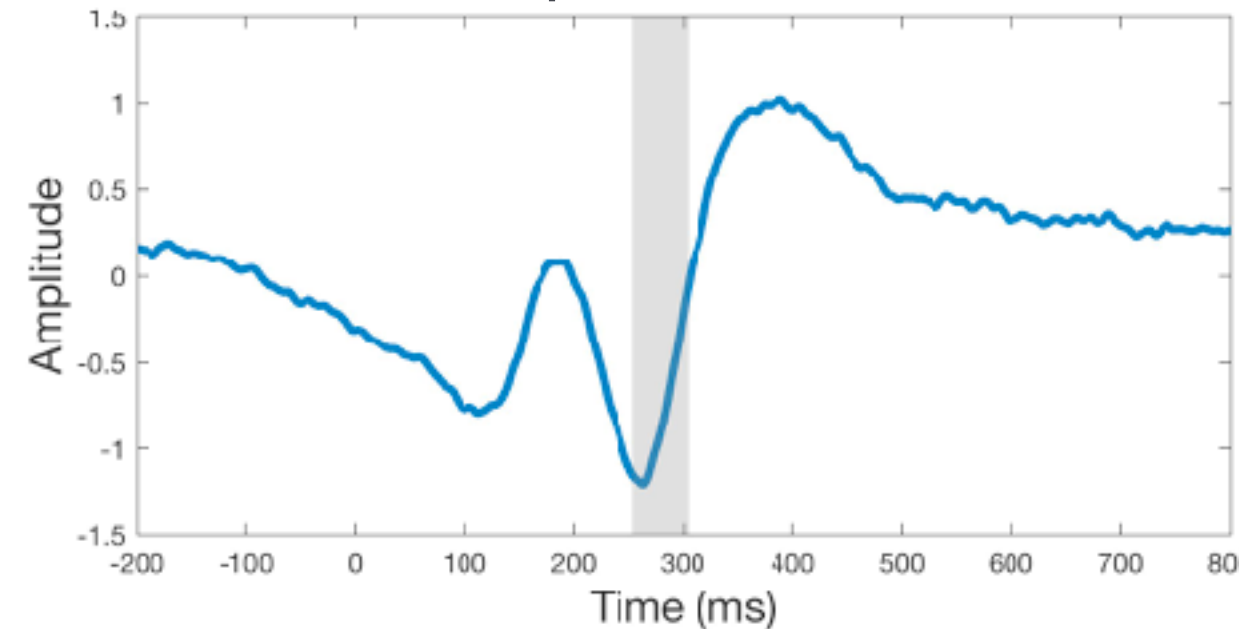


Grand average

GED midfrontal component



GED component time series



GED parameters

R covariance matrix

- computed using all trials, -200 to 0 ms pre-stimulus

S covariance matrix

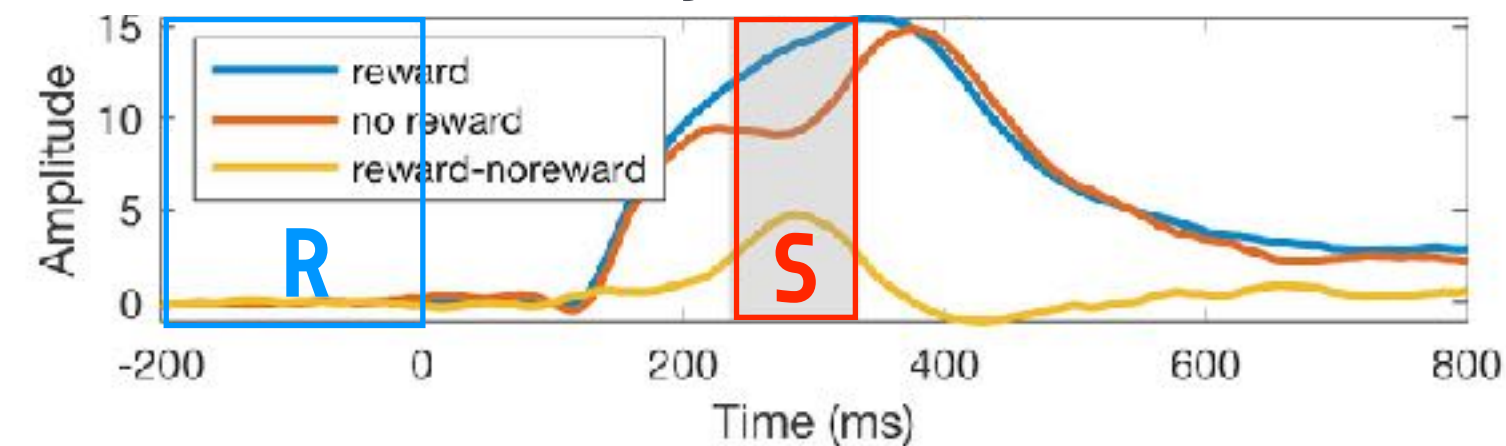
- computed using all trials, 254 to 304 ms post-stimulus

11 GED on real data

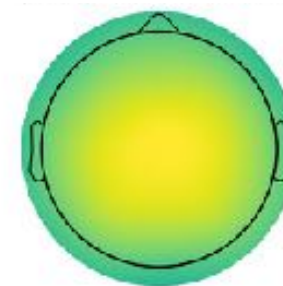
Feedback processing

Lin & Cohen (in prep)

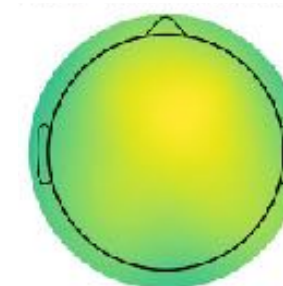
Reward positivity ERP at 235 to 285 ms



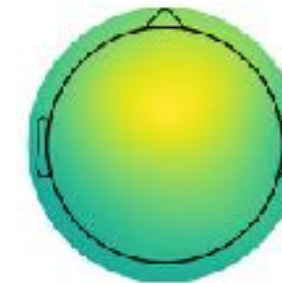
Grand average



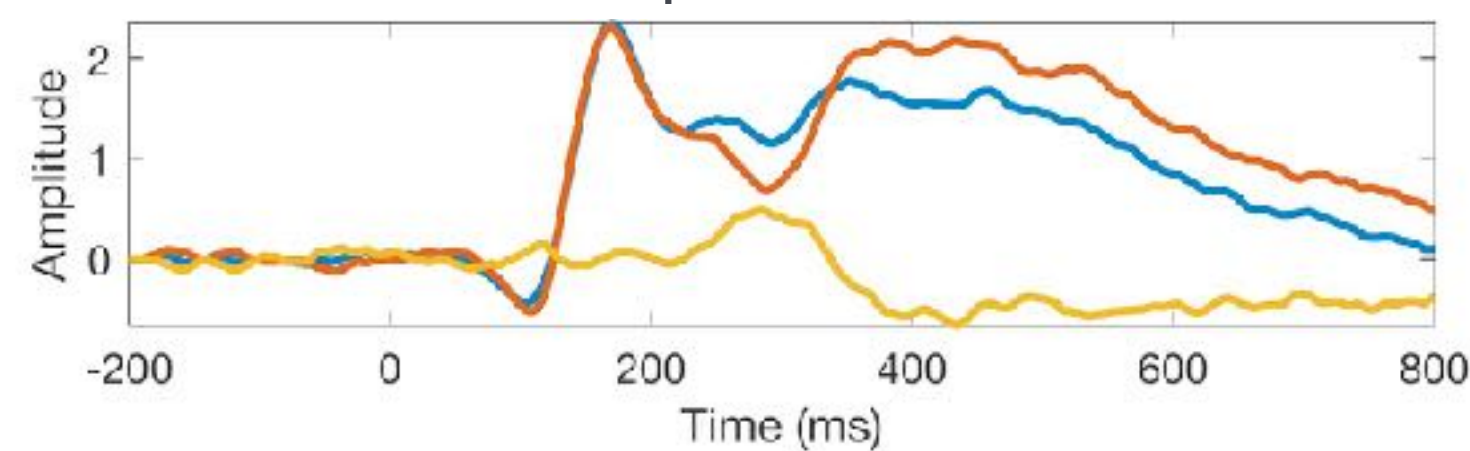
Reward minus no-reward



GED midfrontal component



GED component time series



GED parameters

R covariance matrix

- computed using all trials, -200 to 0 ms pre-feedback

S covariance matrix

- computed using all trials, 235 to 285 ms post-feedback

Generalized eigendecomposition: Flexible multivariate method

Ideal for experimental research (hypothesis testing)

Reduces dimensionality and separates sources (*hypothesis-driven* source-separation)

Components/sources are independent but non-orthogonal (aligns with actual brain dynamics)