Hearing Systems – Part 1 of 3

https://hearingsystems.github.io/

TU Ilmenau – Audio Signal Processing & Audio Systems

18. Januar 2023

Dr. rer. nat. Iko Pieper

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Introduction

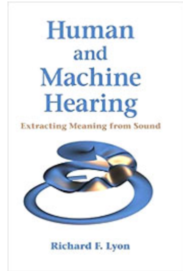
- audifon:
  - audifon GmbH & Co. KG develops, produces and sells hearing systems
  - Headquarter located in Kölleda, Thüringen (also place of production)
  - R&D offices in Köln (Electronics) and Ilmenau (Embedded Software)
  - About 200 employees
- myself:
  - Hobbies: drumming, music production
  - M.Sc. Physik, Ph.D. at Medical Physics Group (Oldenburg)
  - developing audio signal processing algorithms at audifon since Mai 2022

Introduction

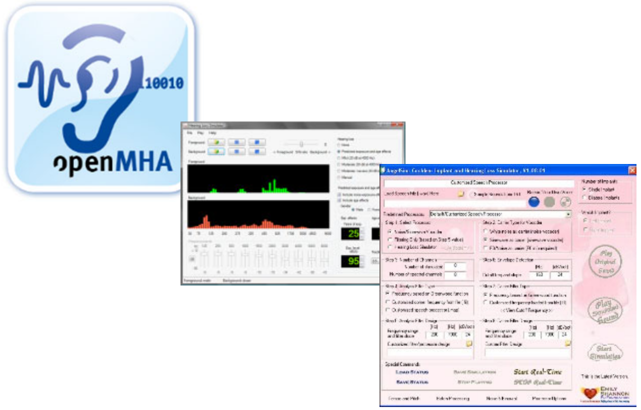
- Three lectures and one seminar.
- Useful links:
  - https://hearingsystems.github.io/,
  - https://moodle2.tu-ilmenau.de/course/view.php?id=4426.
- Topics we will cover today:
  - ***Basics****:* units, hearing, tonotopy, cochlear gain & compression, hearing loss.
- Topics you will cover with Dr. Tamas Harczos:
  - ***Devices:*** hearing aids, cochlear implants, optogenetic stimulation, hearables.
  - ***Technologies:*** audiological features, fitness & medical features, hardware & software.
  - ***Current trends*** in research & development.

Further resources

- Books:
  - *Hörakustik 3.0 - Theorie und Praxis* (Jens Ulrich, Eckhard Hoffmann), ISBN: 978-3-9428-7336-9
  - *Auditory Prostheses: New Horizons* (Zeng, Popper, Fay, eds.), ISBN: 978-1-4419-9434-9
  - *Human and Machine Hearing* (Richard F. Lyon), ISBN: 978-1-1070-0753-6, see draft online

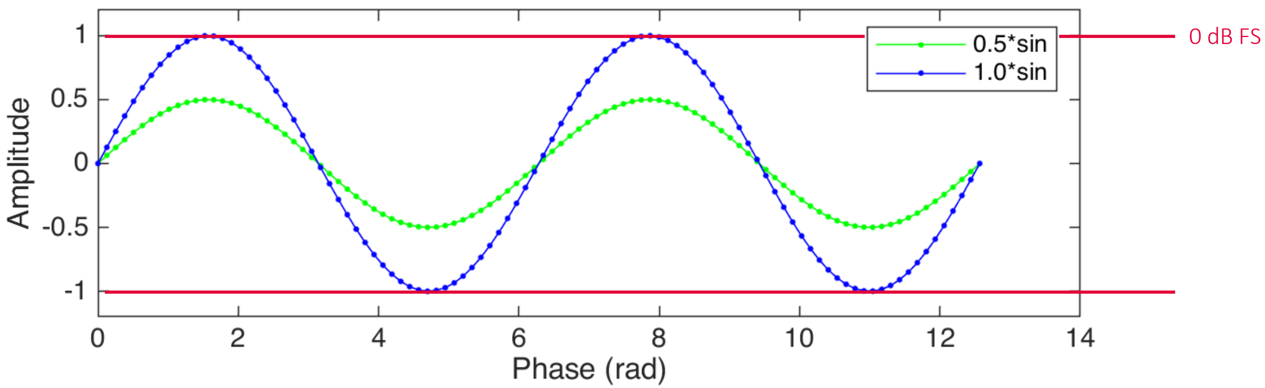


- Programming / Testing:
  - Oldenburg openMHA (Master Hearing Aid)
  - Hearing Loss Simulator (CDC, USA)
  - Cochlear implant (CI) and hearing loss simulator (AngelSim)
  - CI simulation (UT Dallas, USA), CI simulation (UGR, Spain)



Scales and units in audio signal processing

- First of all: Decibel (dB) alone is not a unit, it's a scale. It describes a relationship between two levels.
- Definition for (sound) amplitudes: $A_{dB} = 20 \log_{10}(\mathit{AmplitudeRatio})$, meaning:
  - if AmplitudeRatio = A1 / A2 = **1 / 100** → $20 \log_{10}(1/100) =$ **-40 dB**,
  - if AmplitudeRatio = A1 / A2 = **1 / 10** → $20 \log_{10}(1/10) =$ **-20 dB**,
  - if AmplitudeRatio = A1 / A2 = **1 / 2** → $20 \log_{10}(1/2) =$ -6.02 dB ≈ **-6 dB**.
- The unit **dB FS** (Decibel full scale): A2 is the maximum output of the given system.
  - E.g.: Audio sample amplitudes in MATLAB are in range [-1, +1) → 0 dB FS means |signal| values approach 1.



Further increase in amplitude
→ clipping.

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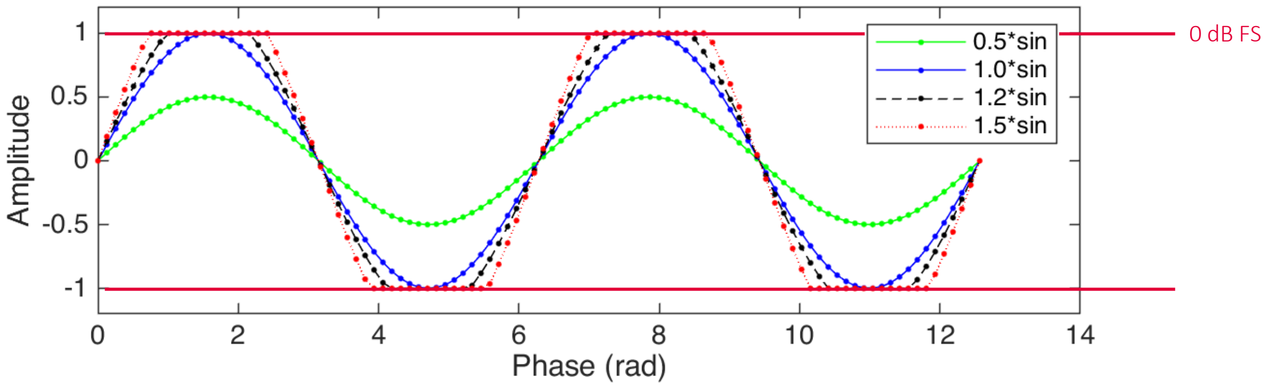

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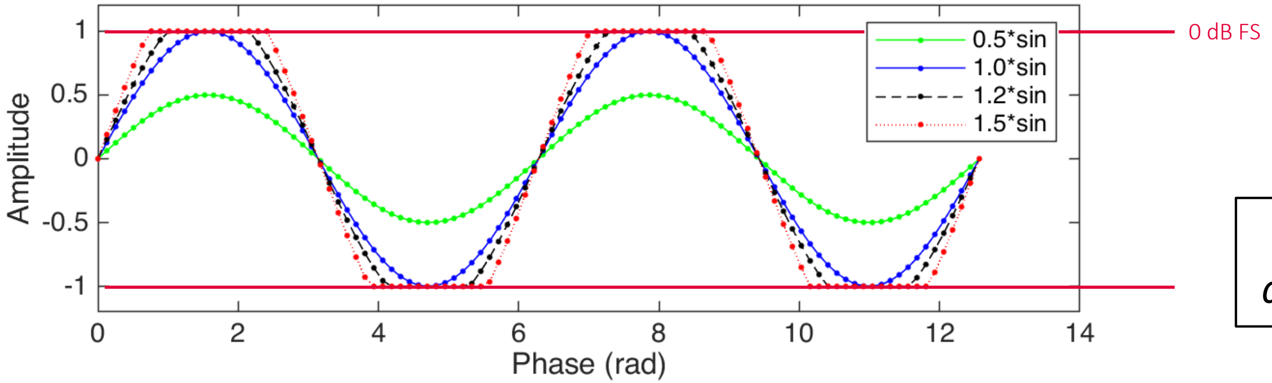

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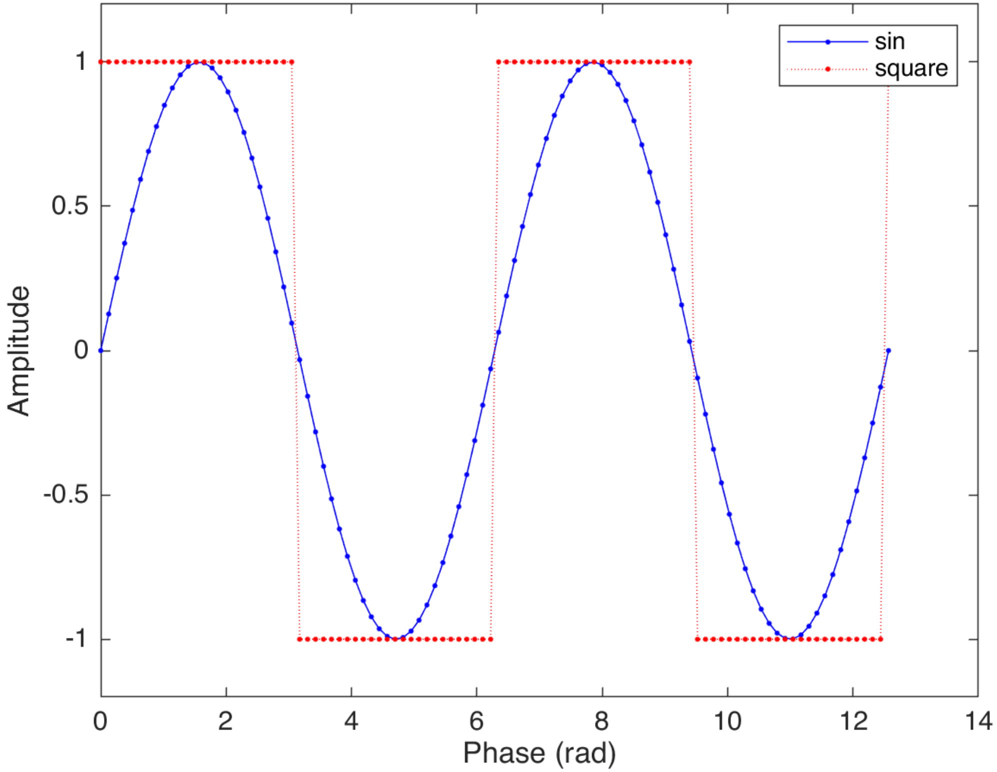
Conversion:
$dB = 20\log_{10}(mag) \Leftrightarrow mag = 10^{(dB/20)}$

•• Scales and units in audio signal processing: dB FS

- The peaks (dB FS) of a signal do not necessarily reveal its impact on “loudness”. Calculating the RMS (root-mean-square) of chunks of samples helps → **signal form matters!**

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max(|square|)= 1.000 = 0.000 dB FS
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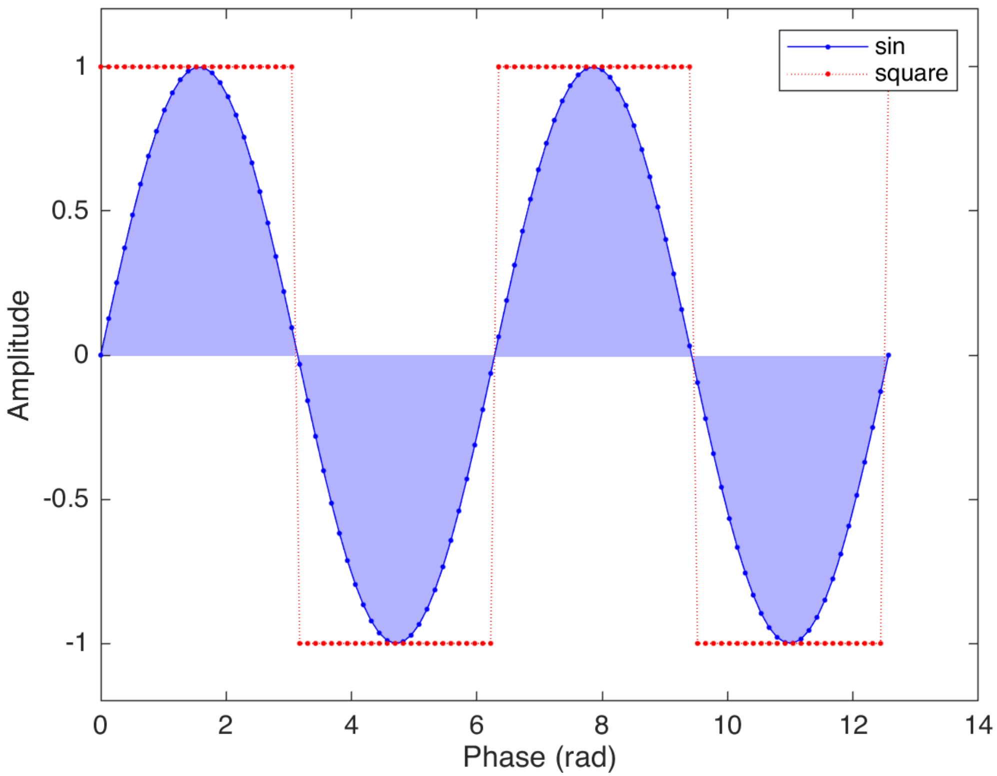

$$RMS = \sqrt{\frac{1}{N}\sum_{n=1}^{N} x_n^2}$$

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max(|square/2|)= 0.500 = -6.021 dB FS

 RMS(sine)  = 0.704 = -3.054 dB FS (RMS)
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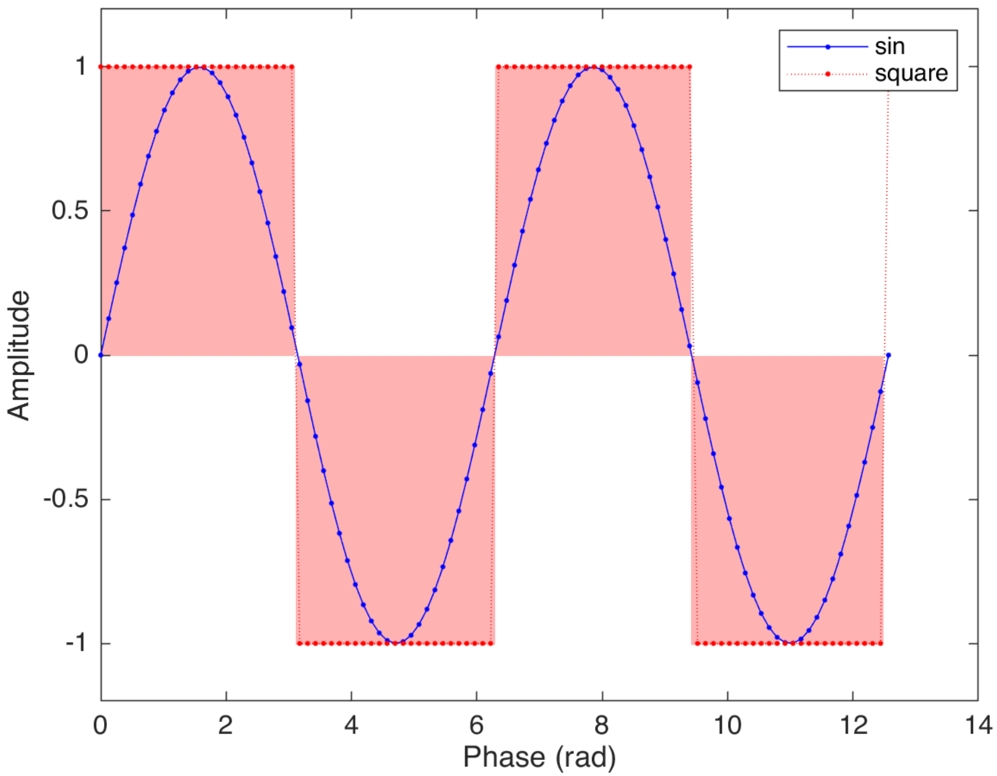

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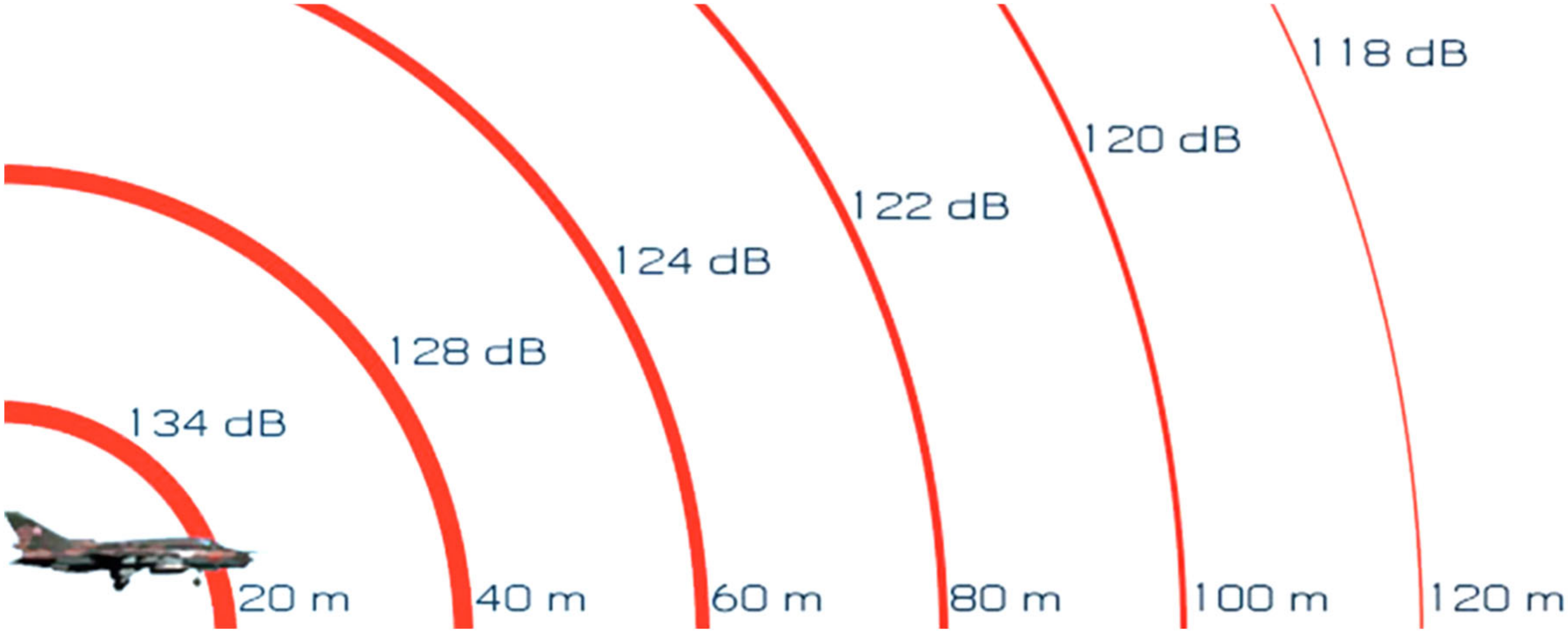
- The unit **dB SPL** (Decibel sound pressure level): relates the RMS of the pressure fluctuations in the air p to the reference sound pressure $p_0 = 20\,\mu\text{Pa}$ (approx. threshold of human hearing for 1 kHz sine). $L_{\text{dB SPL}} = 20 \log_{10} (p/p_0)$.
  - Distance (source to receiver) is important, 1 m is frequently used as standard distance.
  - Doubling the distance halves the pressure in free field (-6 dB SPL).



Source: https://www.translatorscafe.com/unit-converter/ZH/sound-pressure-level/

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  - Doubling the distance halves the pressure in free field (-6 dB SPL).
  - Typical ranges:
    - **20-30 dB SPL**: very calm room,
    - **40-60 dB SPL** (1 m): normal conversation,
    - **70-90 dB SPL** (10 m): nearby heavy traffic, **>90 dB SPL: Hearing damage over long-term exposure**
    - **100-110 dB SPL** (1 m): jack hammer / chain saw,
    - **120 dB SPL** (100 m): jet engine, **>120 dB SPL: Instantaneous noise-induced hearing loss**
    - **194 dB SPL**: largest pressure fluctuation an undistorted sound wave can have in Earth's atmosphere.

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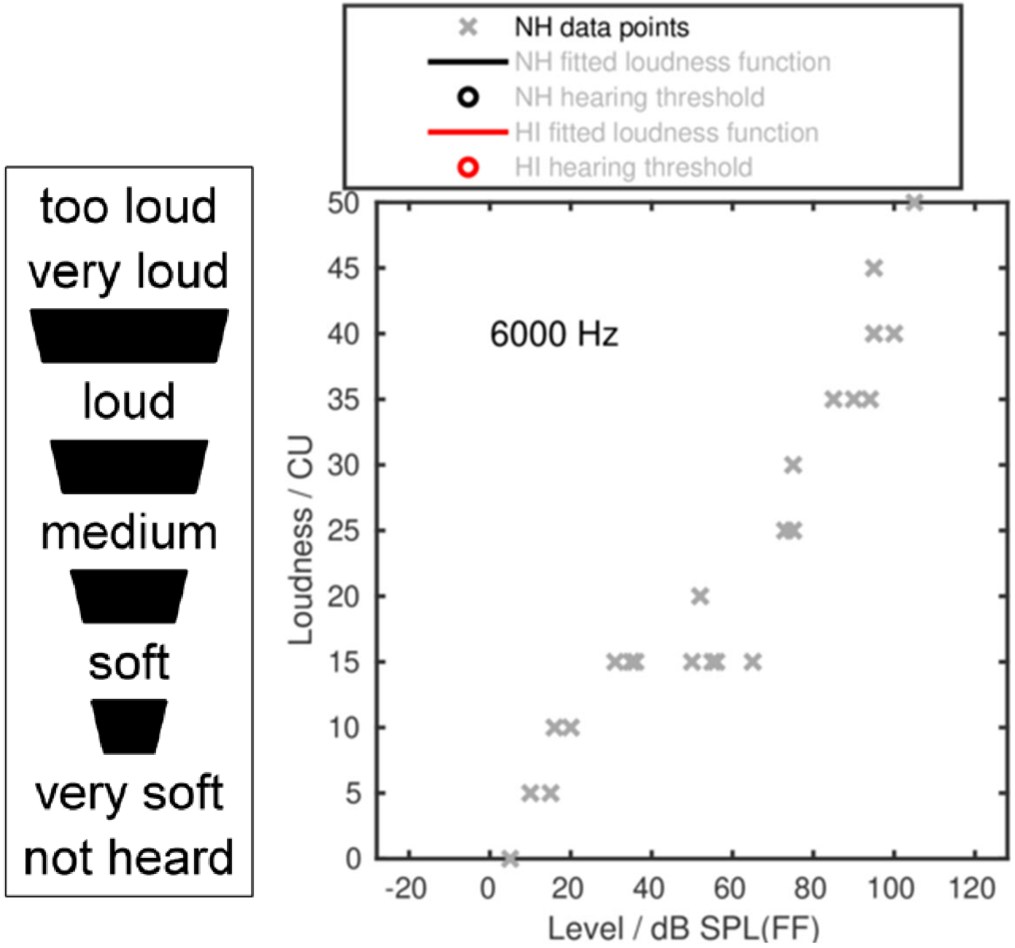
•• Scales and units in audio signal processing: Categorical loudness scaling



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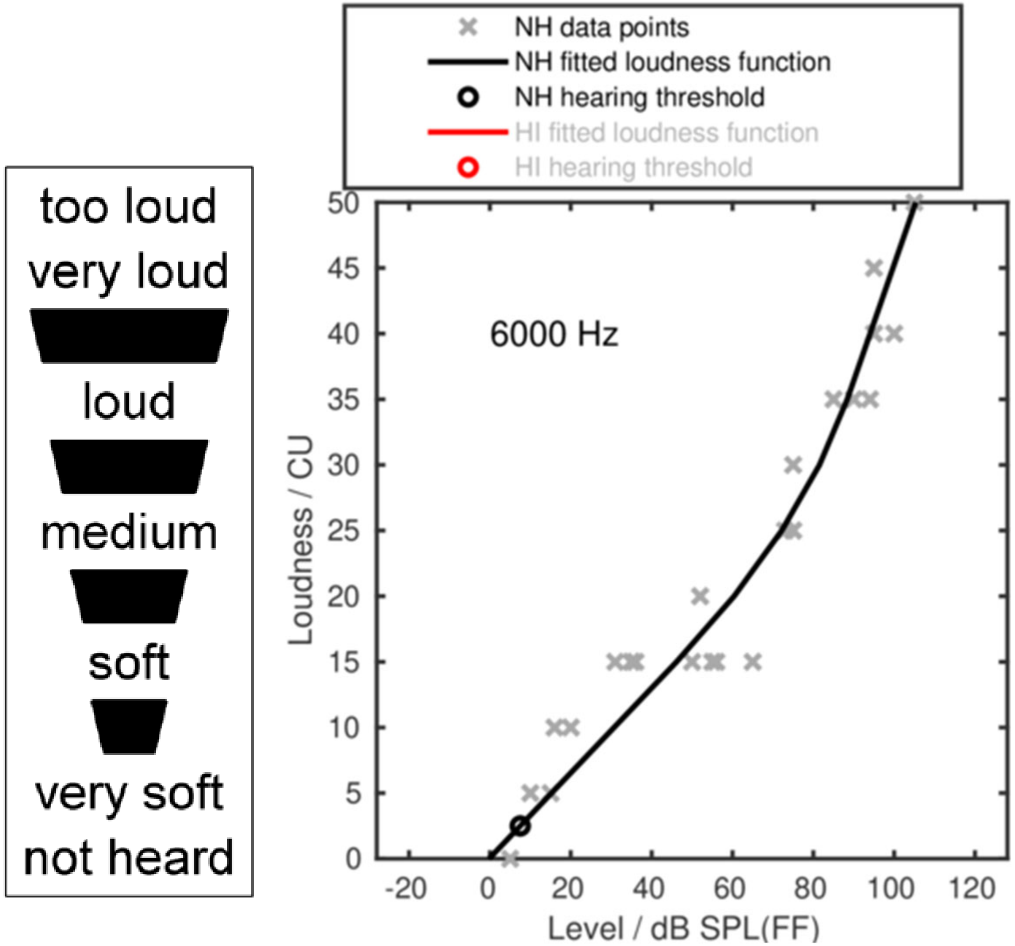

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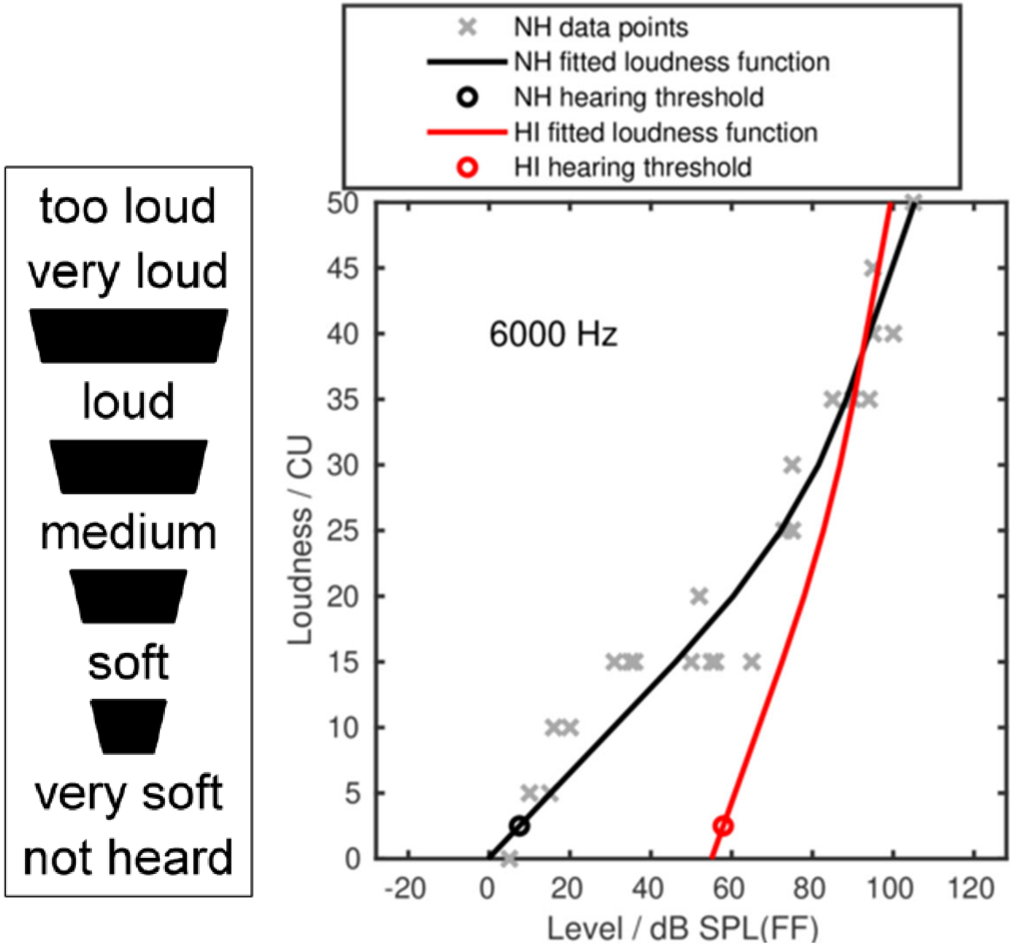
Often observed in case of sensorineural hearing impairment:

- Hearing threshold shifted to higher sound pressure levels
- Uncomfortable level (perceived as too loud, 50 CU) not shifted



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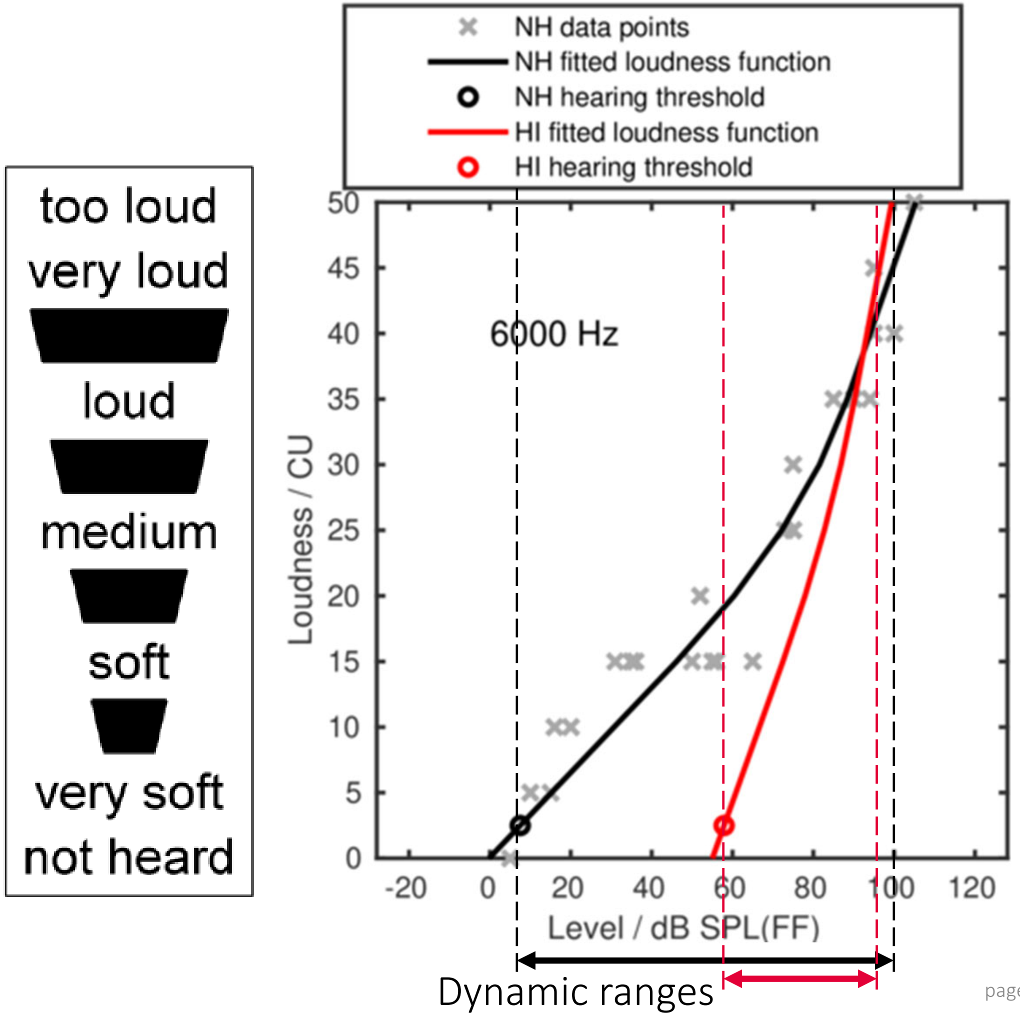
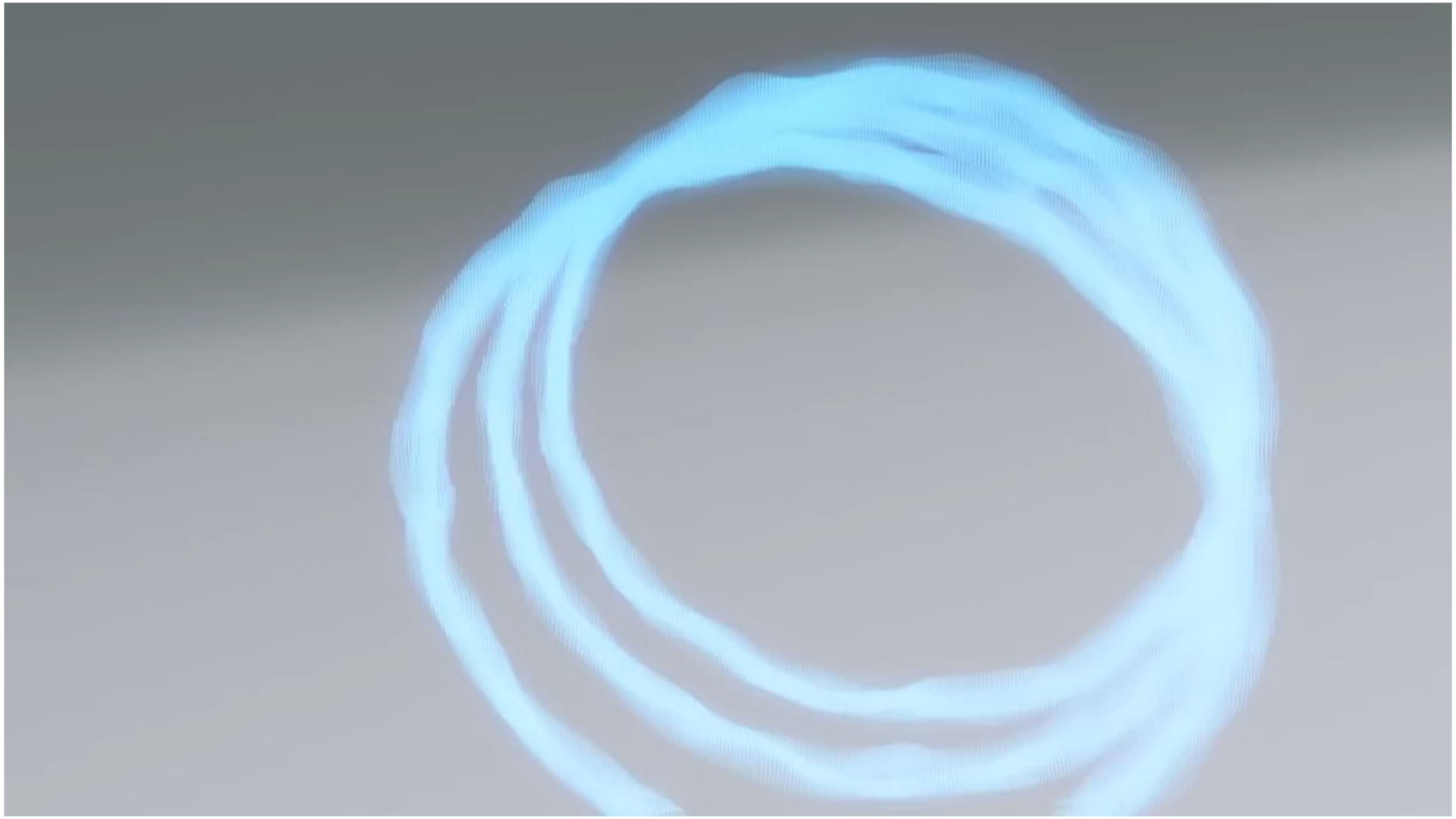
⇒Reduced dynamic range



•• How hearing works

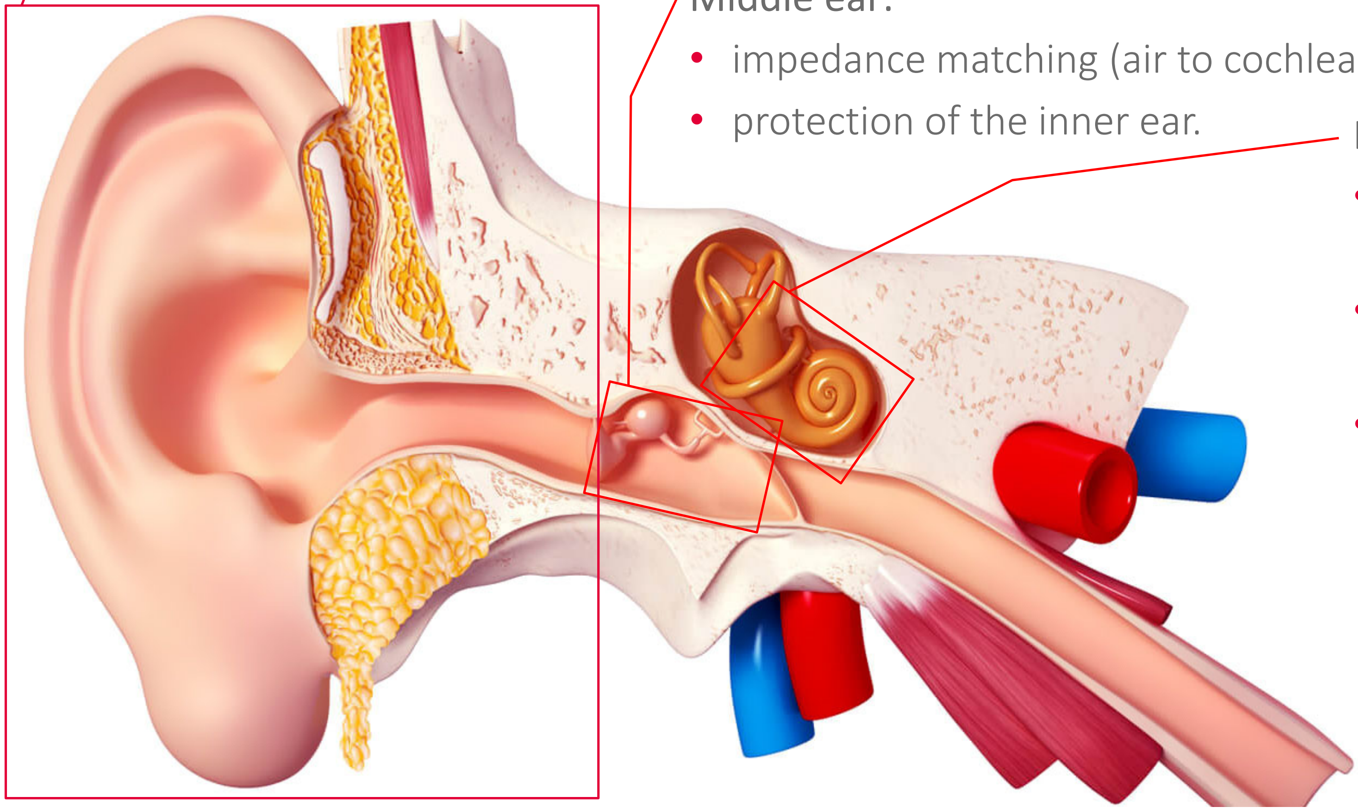


•• Overview

Outer ear: amplification, direction-dependent filtering.

Middle ear:
- impedance matching (air to cochlea),
- protection of the inner ear.

Inner ear (cochlea):
- spectral decomposition of signal (~filter bank),
- extension of dynamic range (compressive nonlinearity),
- transformation into electrical signals.



Source: www.lobe.ca, 2021.

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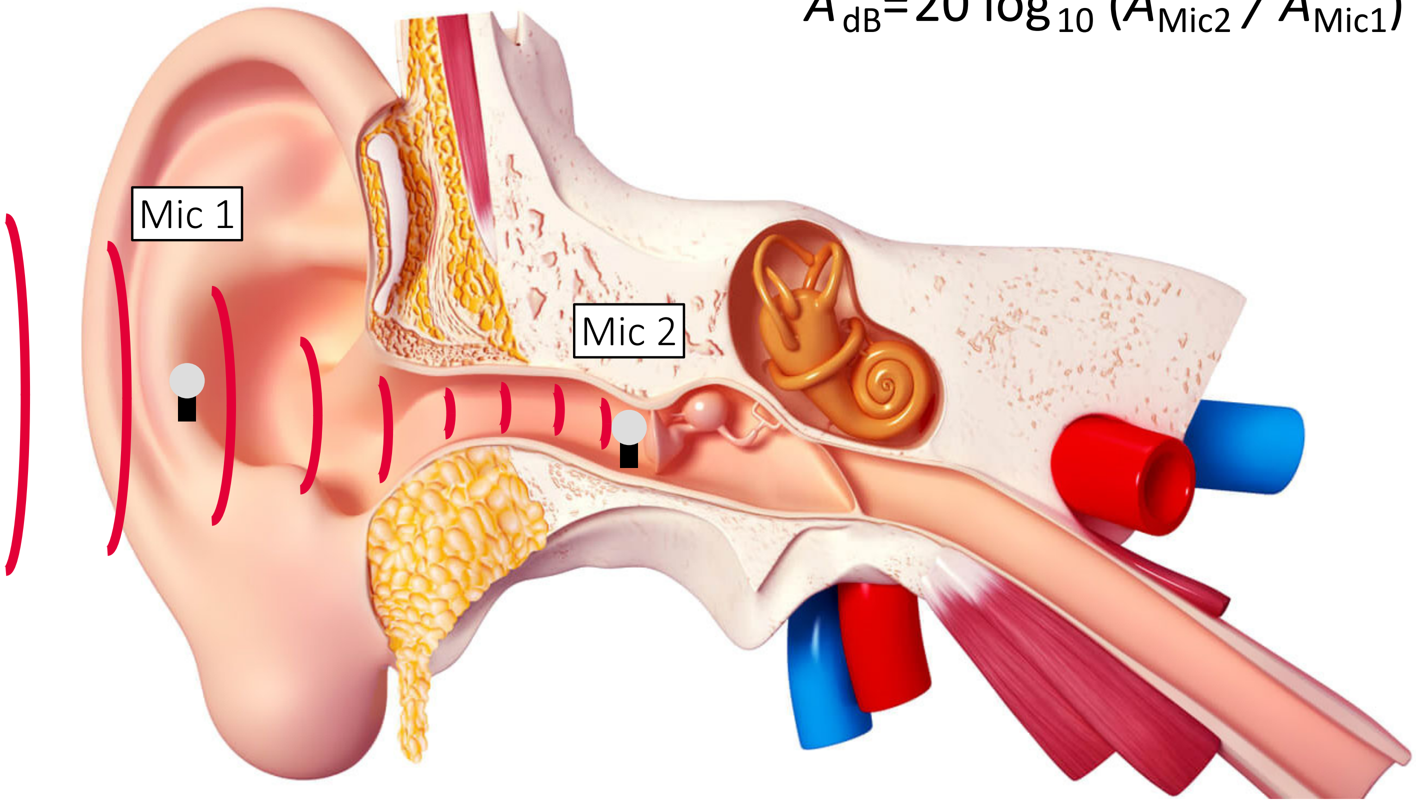
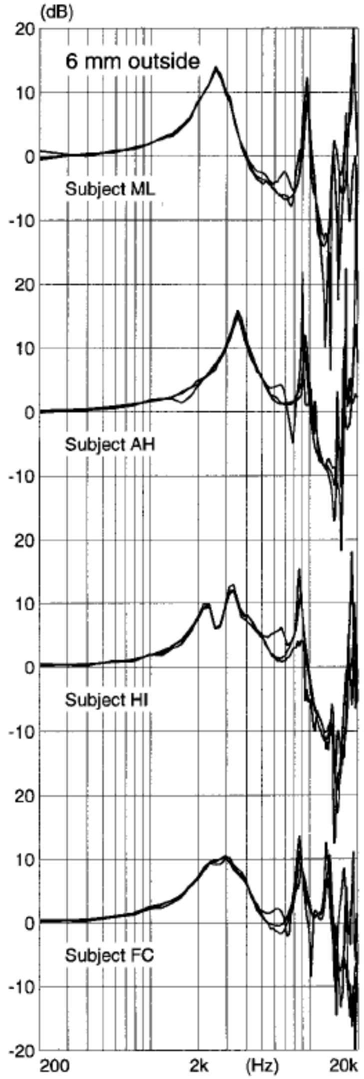
•• Outer ear: Transfer function

$$A_{dB}=20\log_{10}\left(A_{Mic2}/A_{Mic1}\right)$$





Source: Hammershoi, D. and Moller, H.: Sound transmission to and within the human ear canal, 1995

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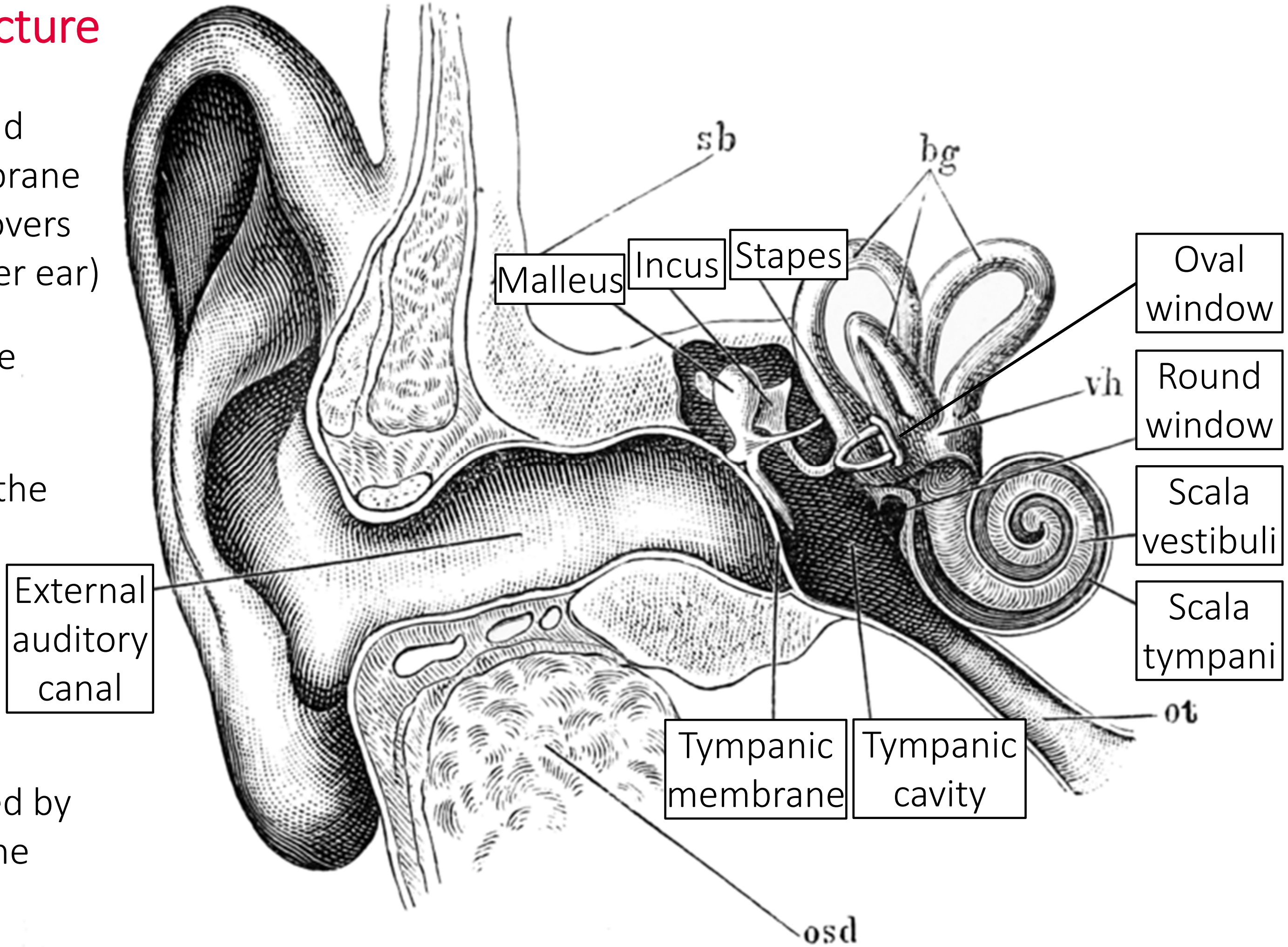
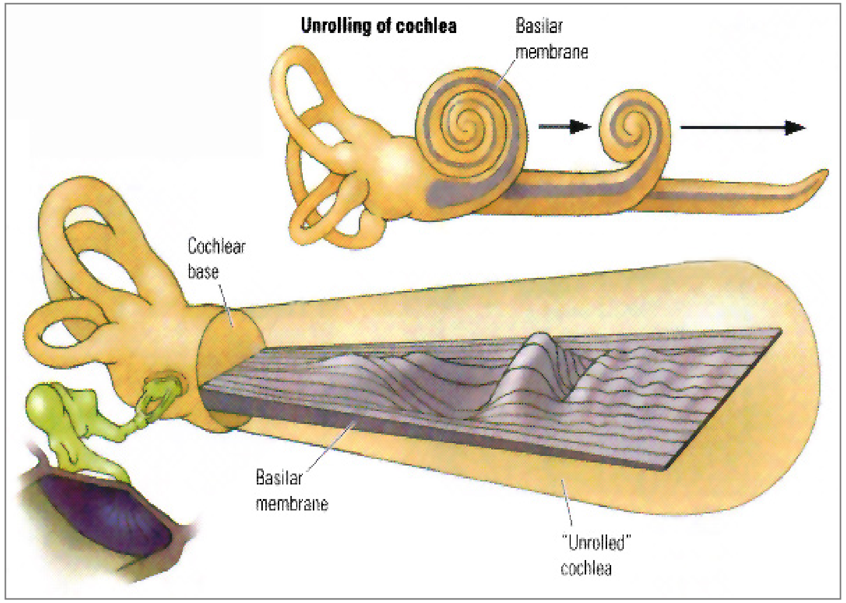
Middle ear and Inner ear: Structure

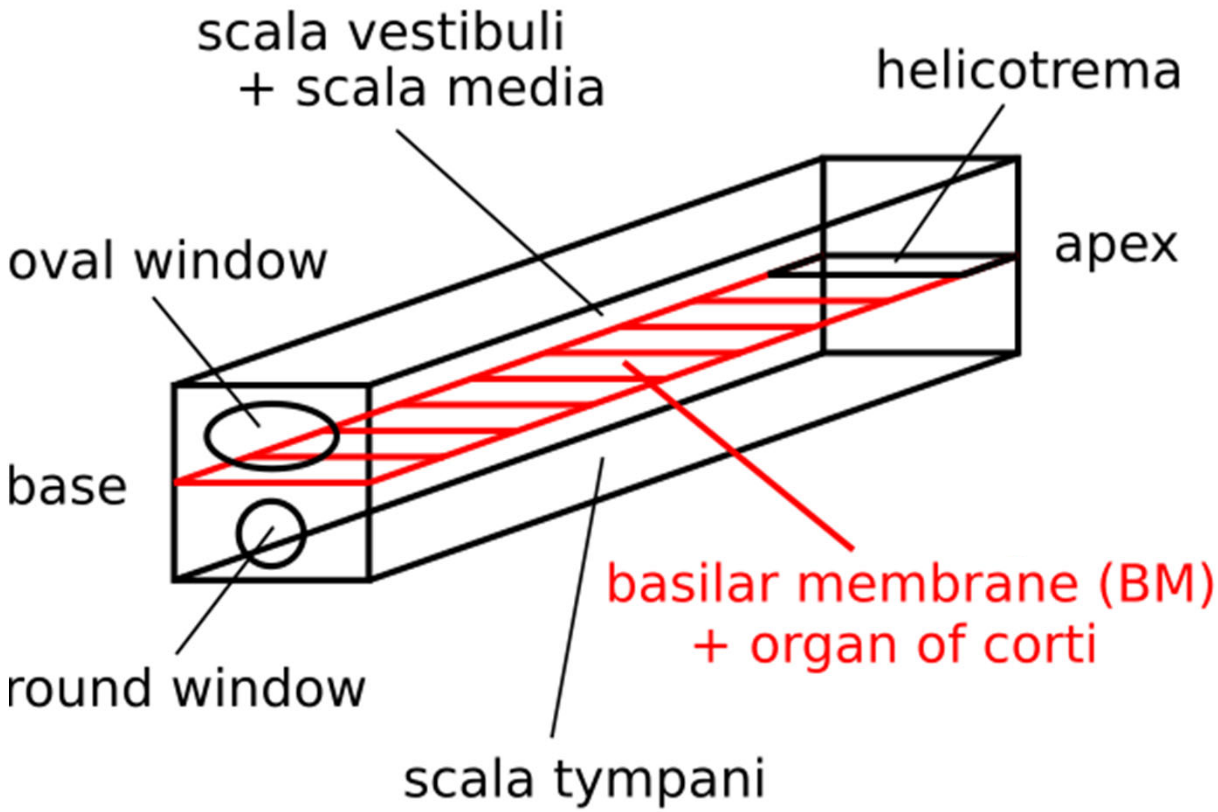
- The three ossicles (maleus, incus, and stapes) connect the tympanic membrane (ear drum) to the membrane that covers the oval window of the cochlea (inner ear)
- The oval window is an opening of the scala vestibuli
- The round window is an opening of the scala tympani, and covered with a membrane as well
- The cochlea scales are filled with fluids
- The cochlea scales are only separated by the basilar membrane that carries the inner and outer hair cells



•• Inner ear (cochlea): Simplified geometry



Source: http://www.pc.rhul.ac.uk



•• Inner ear (cochlea): Impedance

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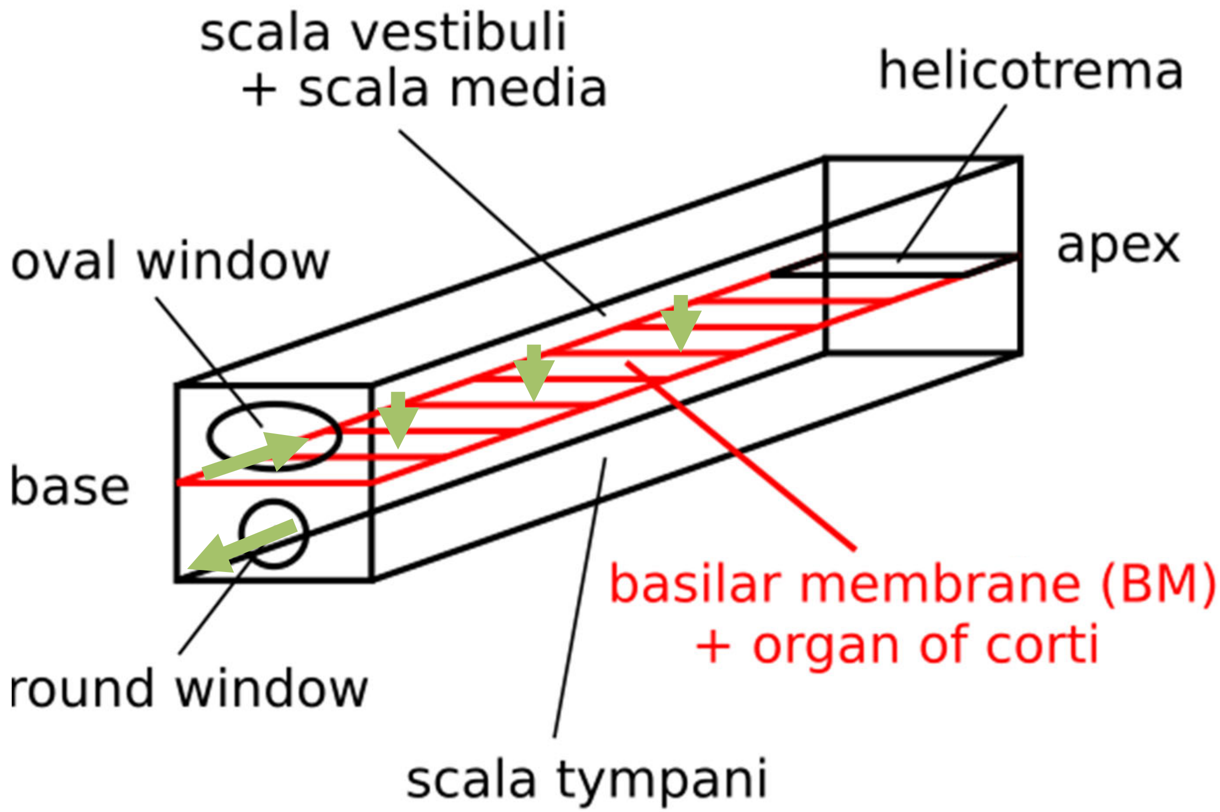


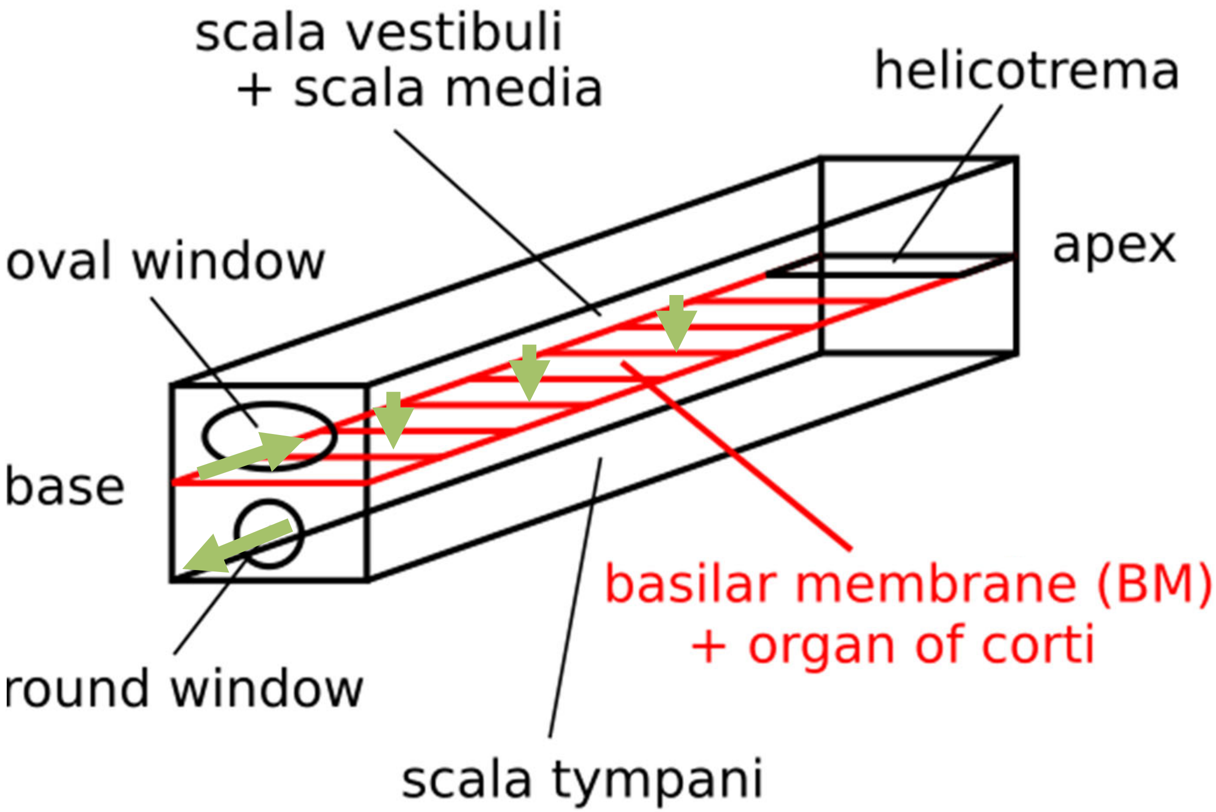
•• Inner ear (cochlea): Impedance

- The mechanical impedance of the cochlea is a combination of...

  ... the stiffness of the membranes inside the cochlea and the membranes covering the oval and round window,
  ... the inertia of the fluids,
  ... the compressibility of the fluids (negligible),
  ... some damping here and there.

- The impedance of this system is lower than the impedance of fluids but still higher than the impedance of air

⇒Impedance matching between air and cochlea is required to avoid reflection of sound waves at the oval window

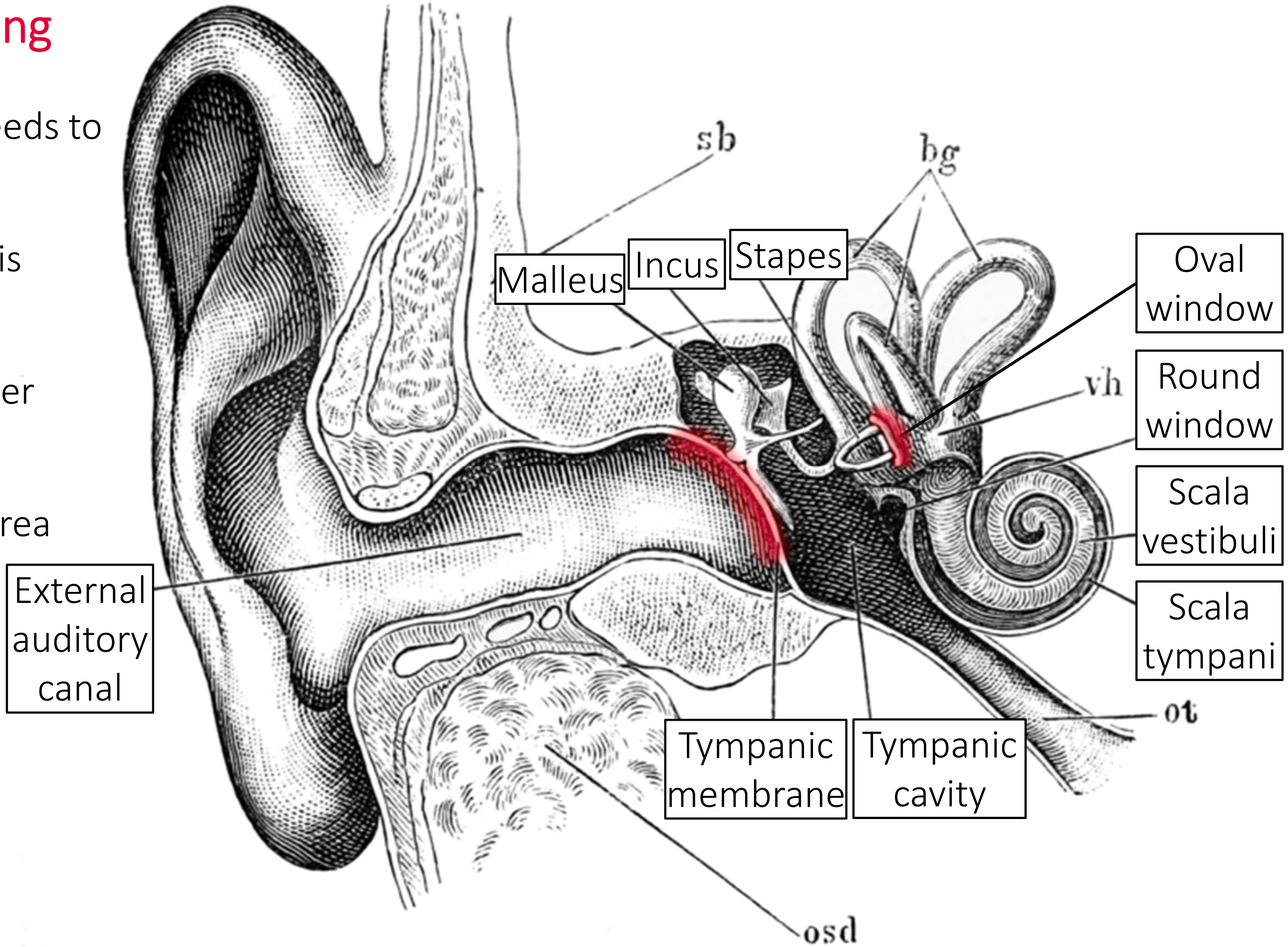


•• Middle ear: Impedance matching

- The sound pressure (force / area) needs to be increased
- A lever could increase the force but is nowhere to be found
- The area of the oval window is smaller than the area of the ear drum

⇒Force is concentrated on a smaller area

⇒Pressure (force / area) is increased



Source: Henry Gray: Anatomy of the human body, Lea & Febiger, 1878

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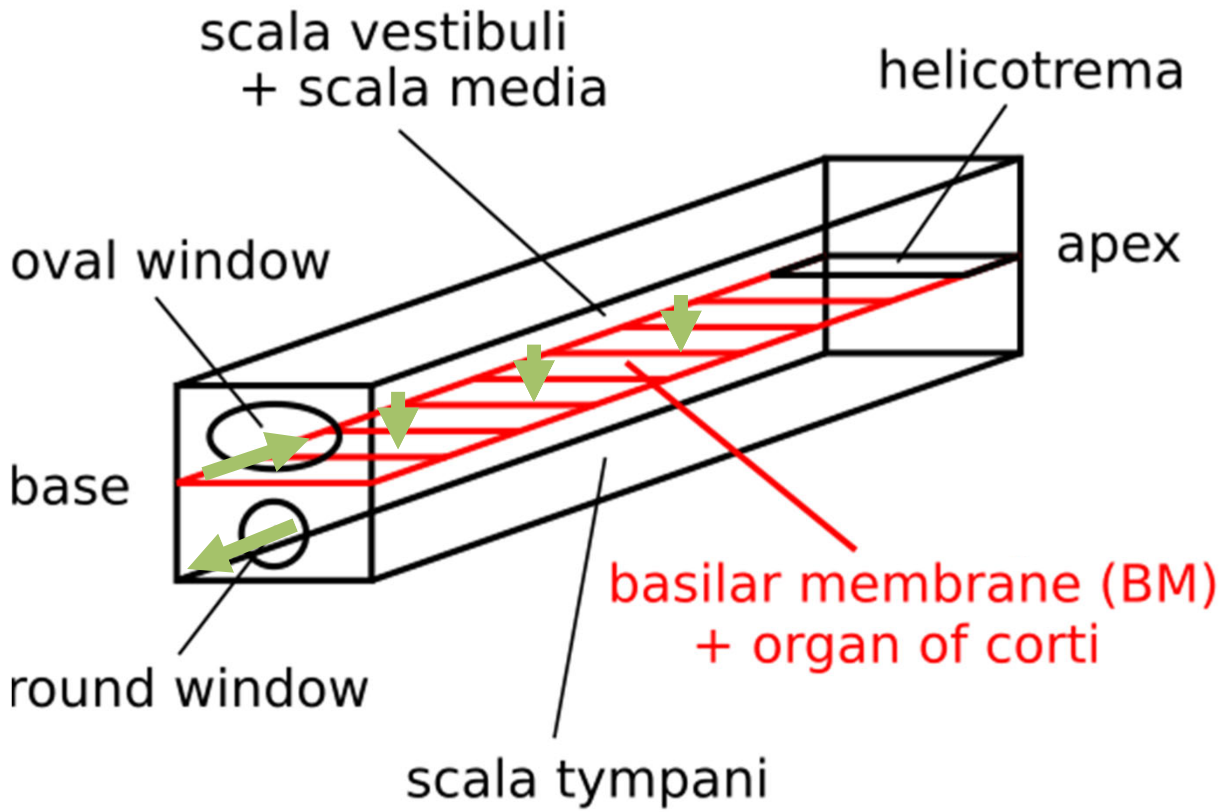
Inner ear (cochlea): Frequency-place transformation

- Stiffness of basilar membrane (BM) decreases from base to apex
- Mass of fluid that needs to be moved increases from base to apex

⇒Resonance frequency decreases from base to apex

⇒High frequency components excite the BM closer to the base, low frequency components closer to the apex

⇒The inner ear is a mechanical spectral analyzer



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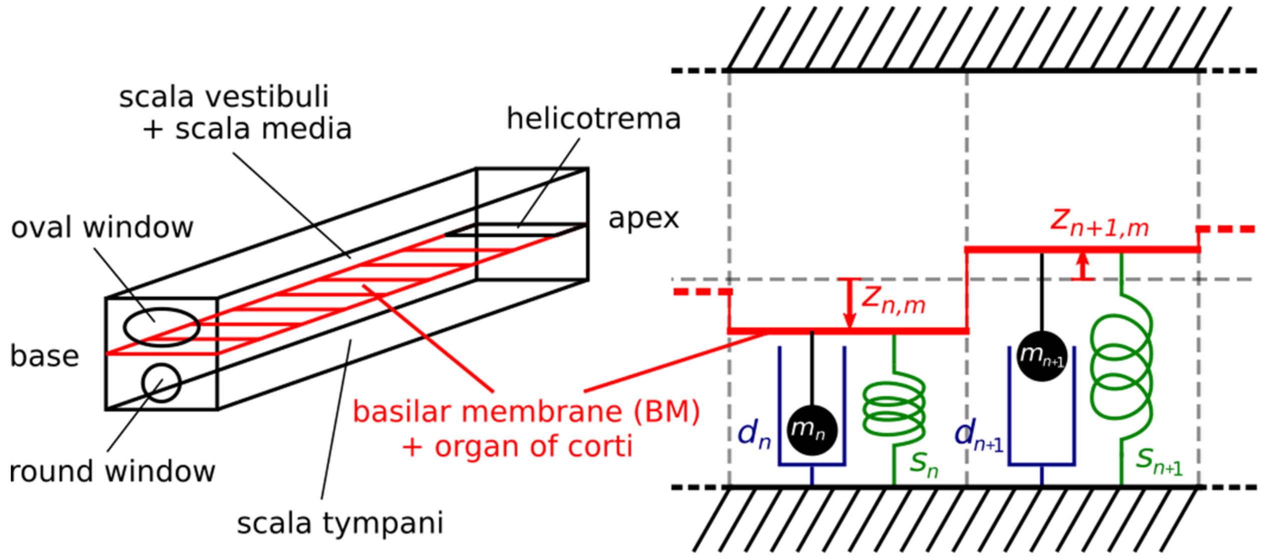

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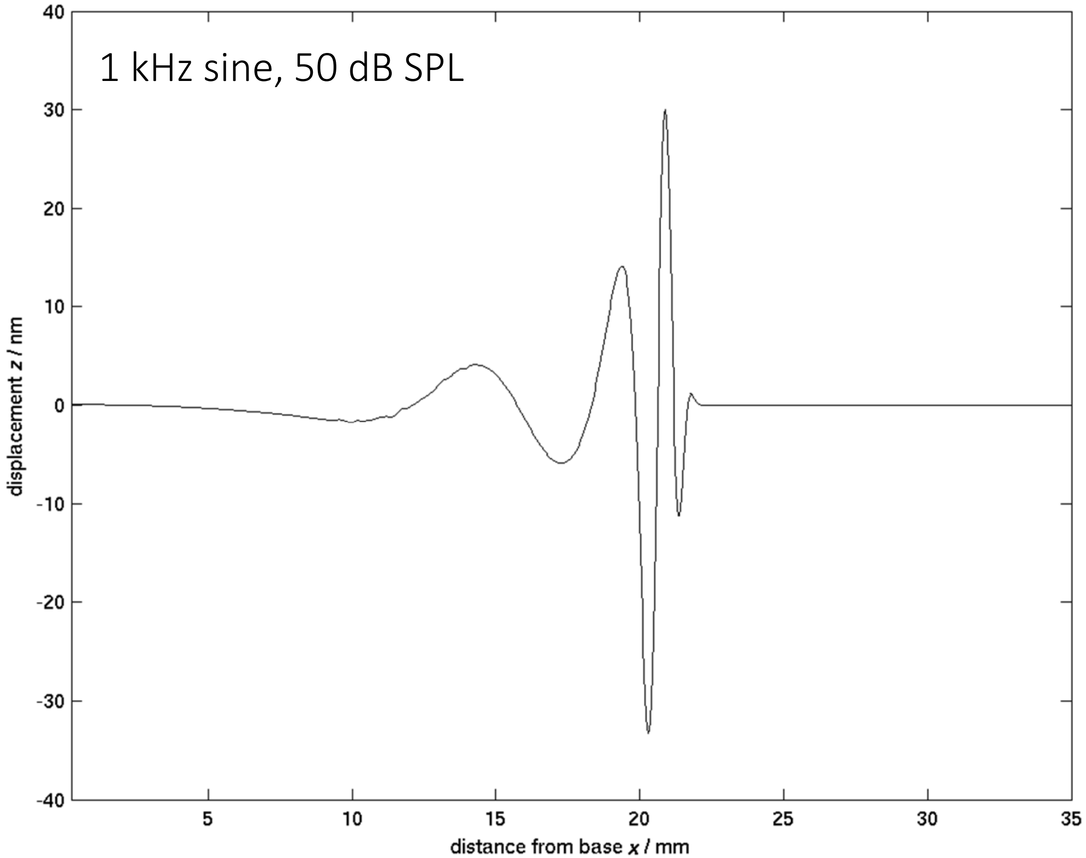

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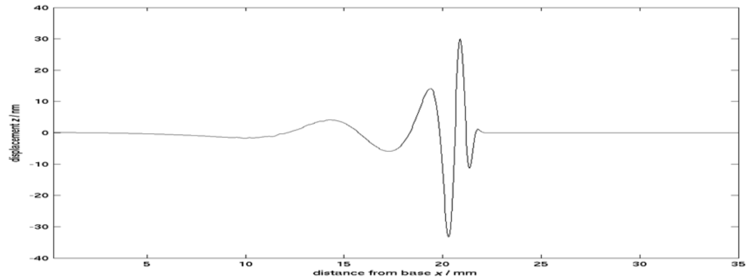
Békésy György, 1899-1972
Biophysicist
Nobel-prize 1961 awardee



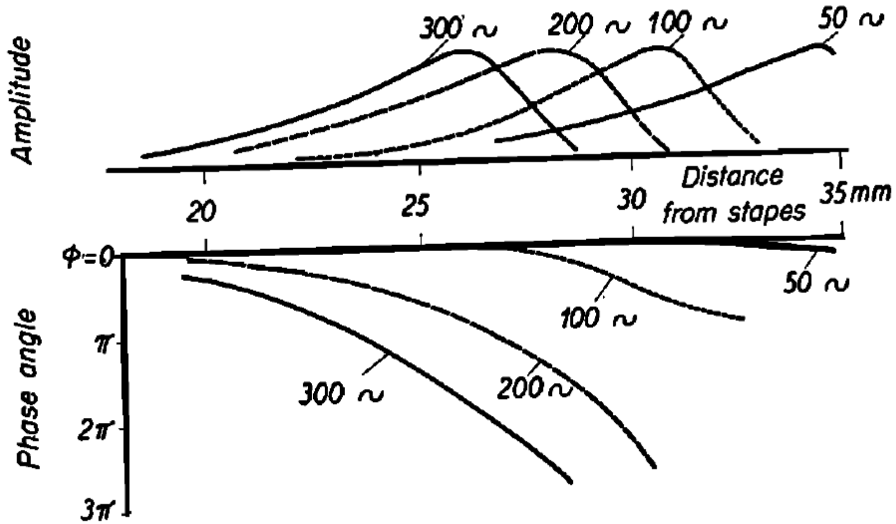


FIG. 5. Amplitude and phase angle at various distances along the cochlear partition. Distance is given from the stapes. Measurements are shown for four frequencies.

Source: Georg V. Békésy: The Variation of Phase Along the Basilar Membrane with Sinusoidal Vibrations, 1947

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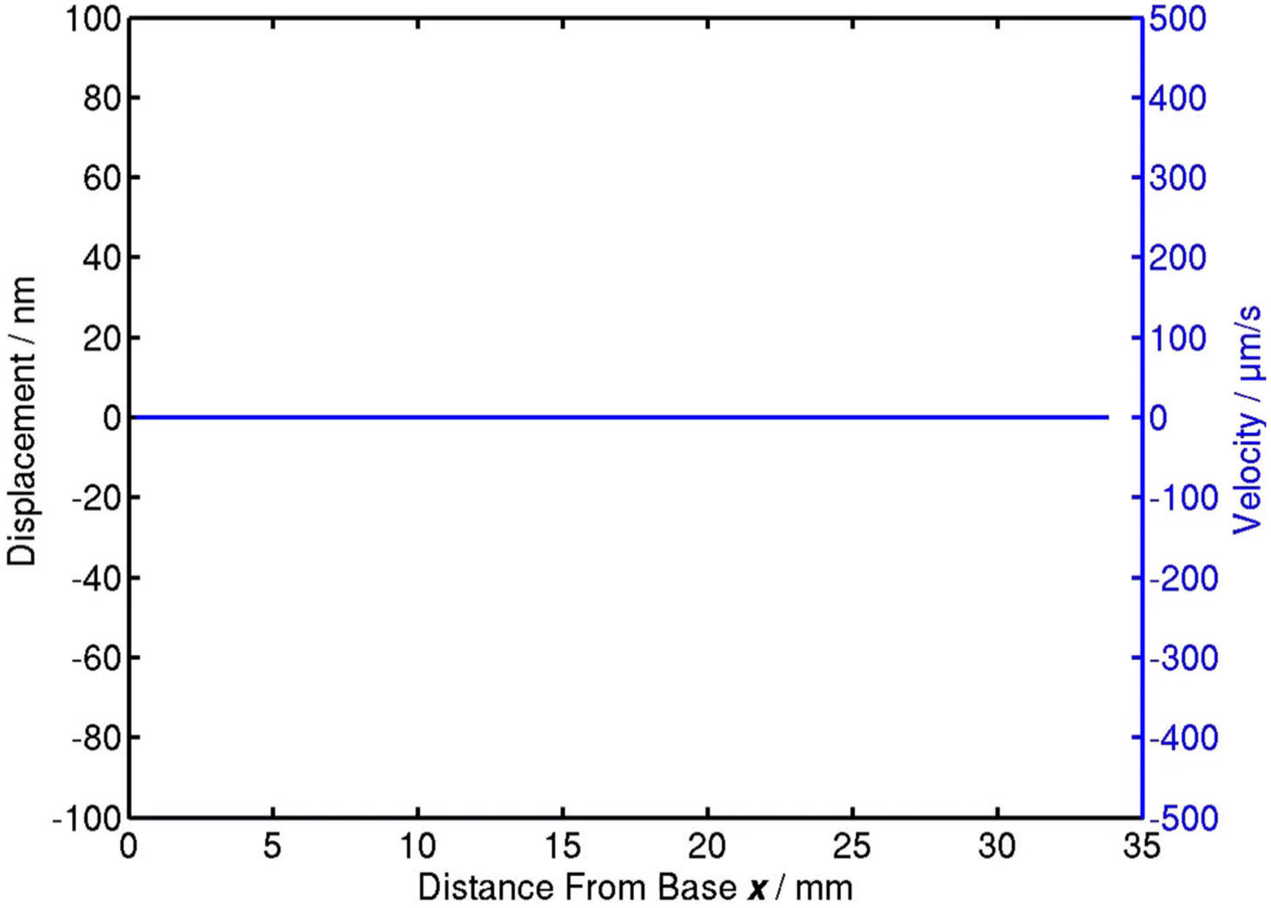

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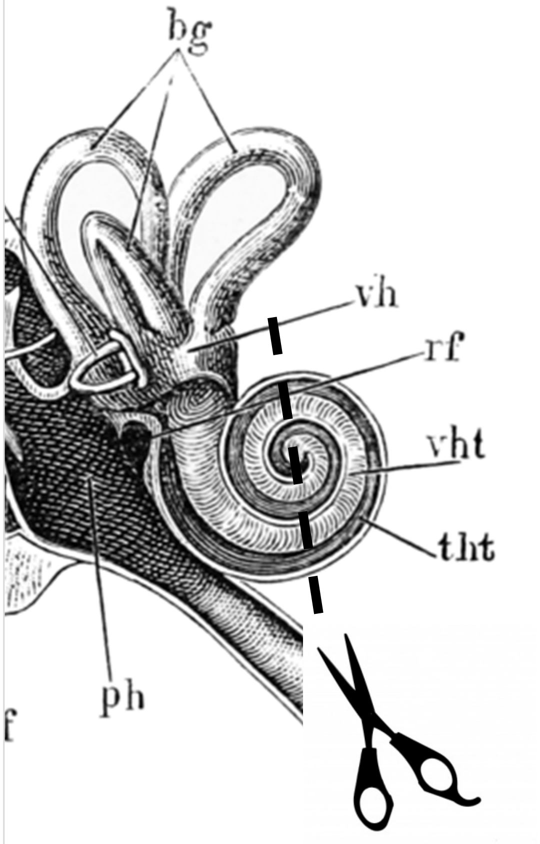

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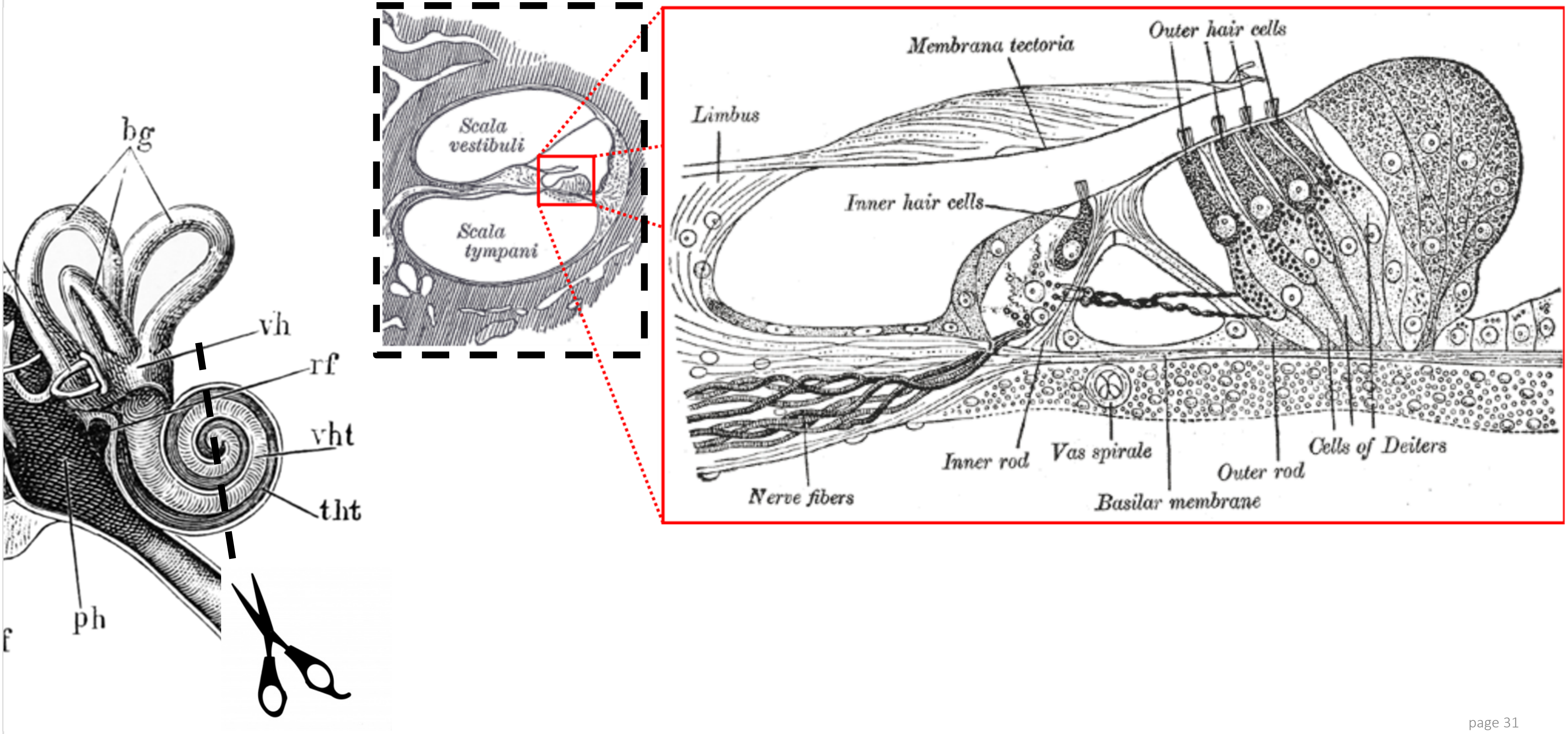

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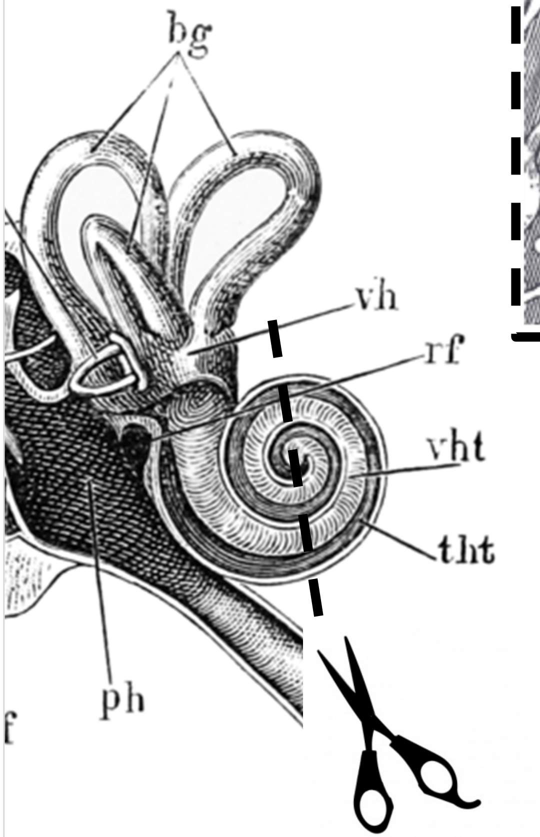
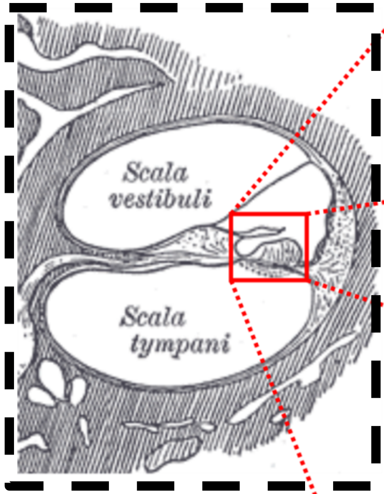
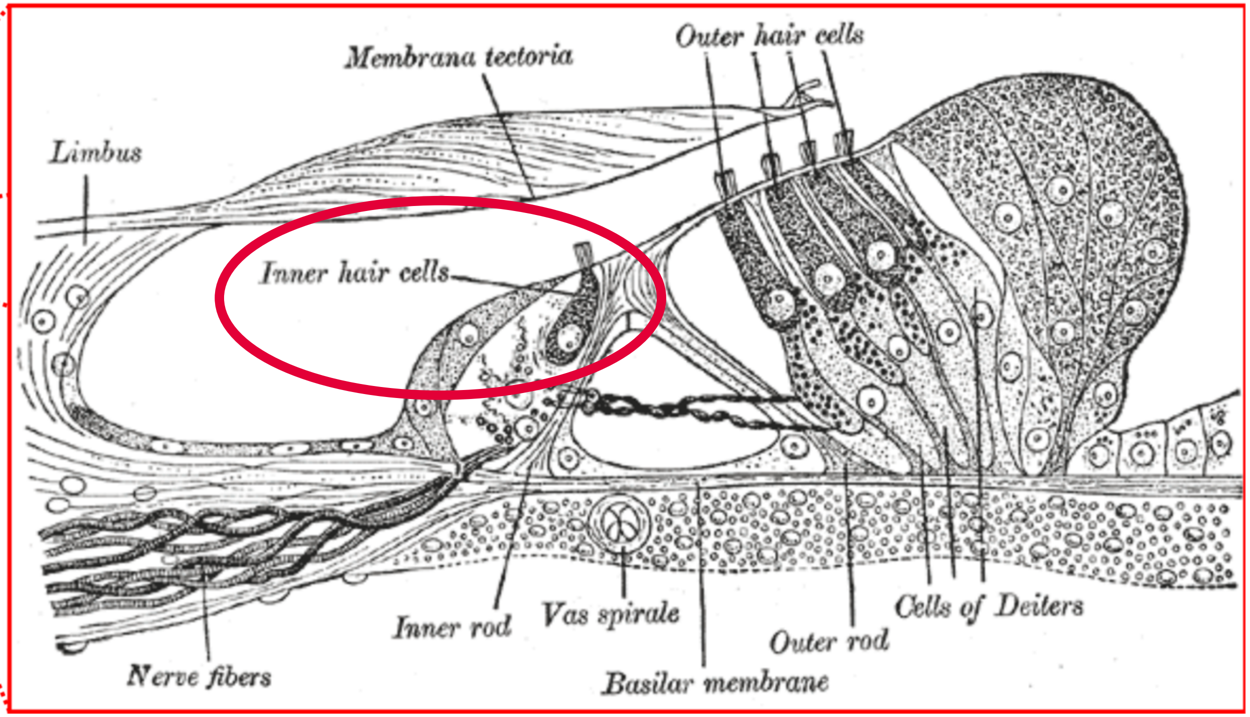
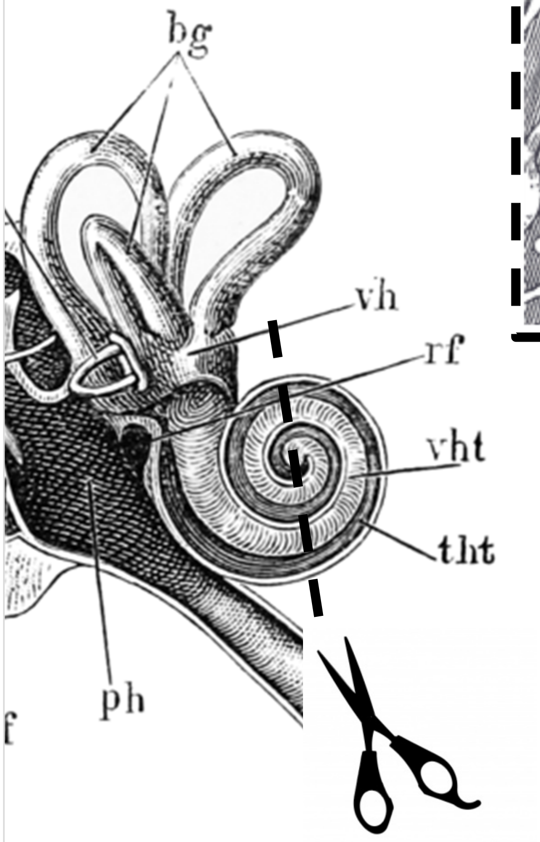
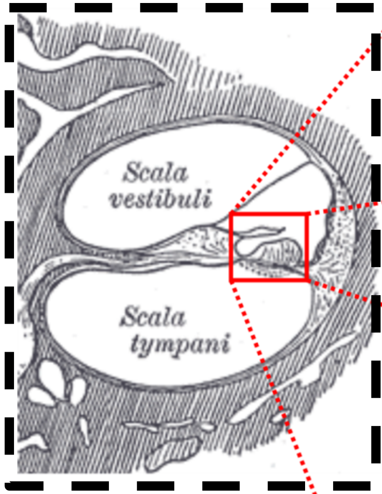


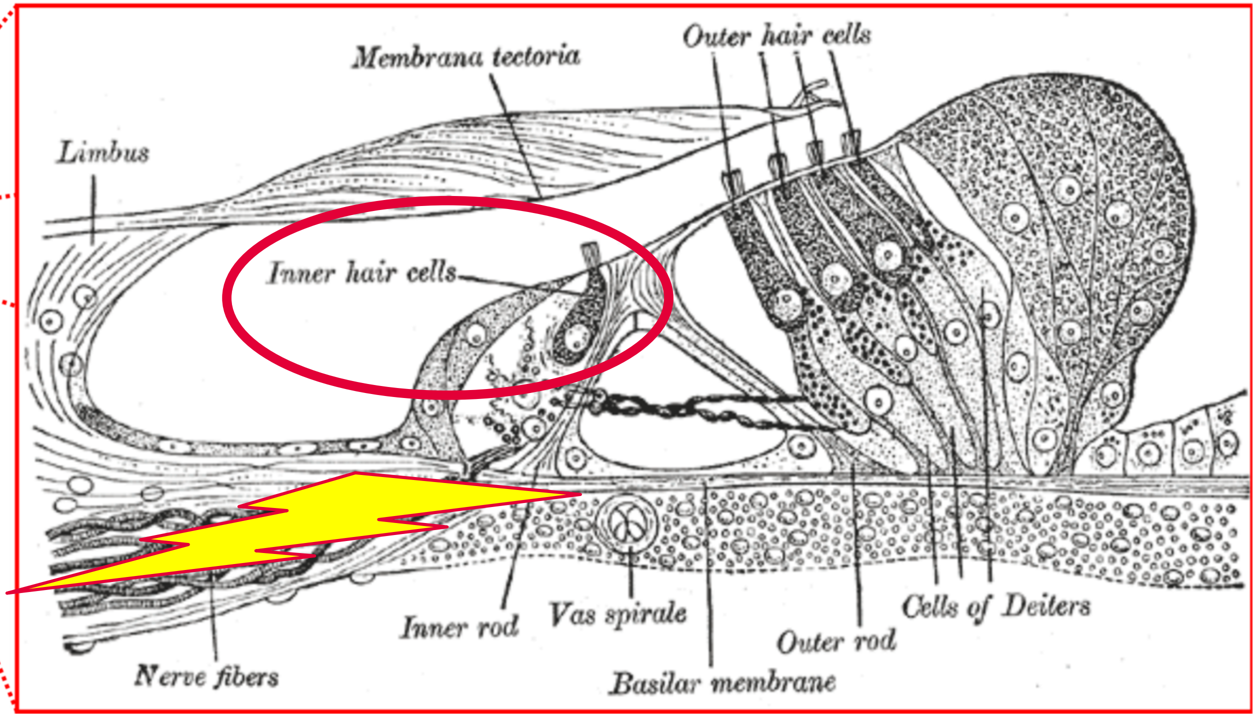




•• Inner ear (cochlea): Inner hair cells



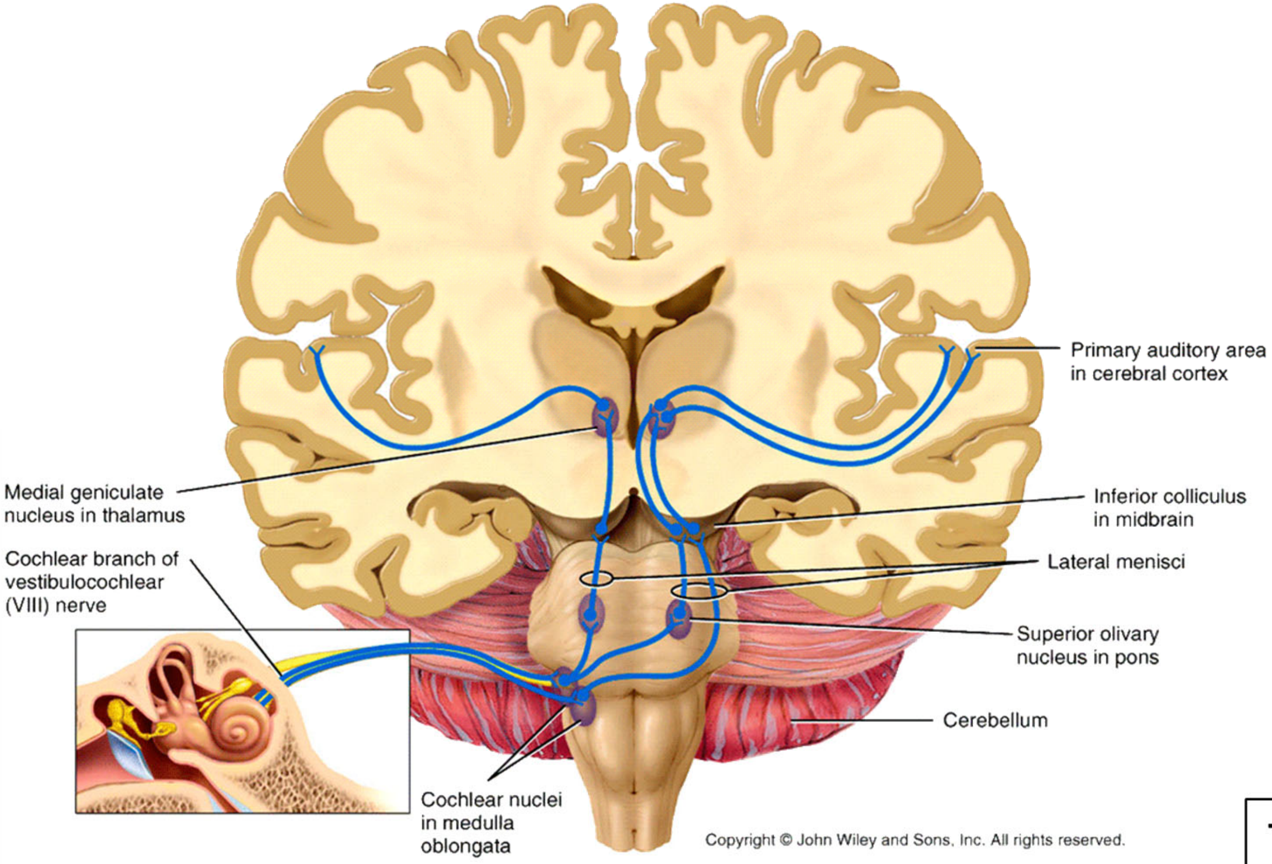




Inner hair cells:

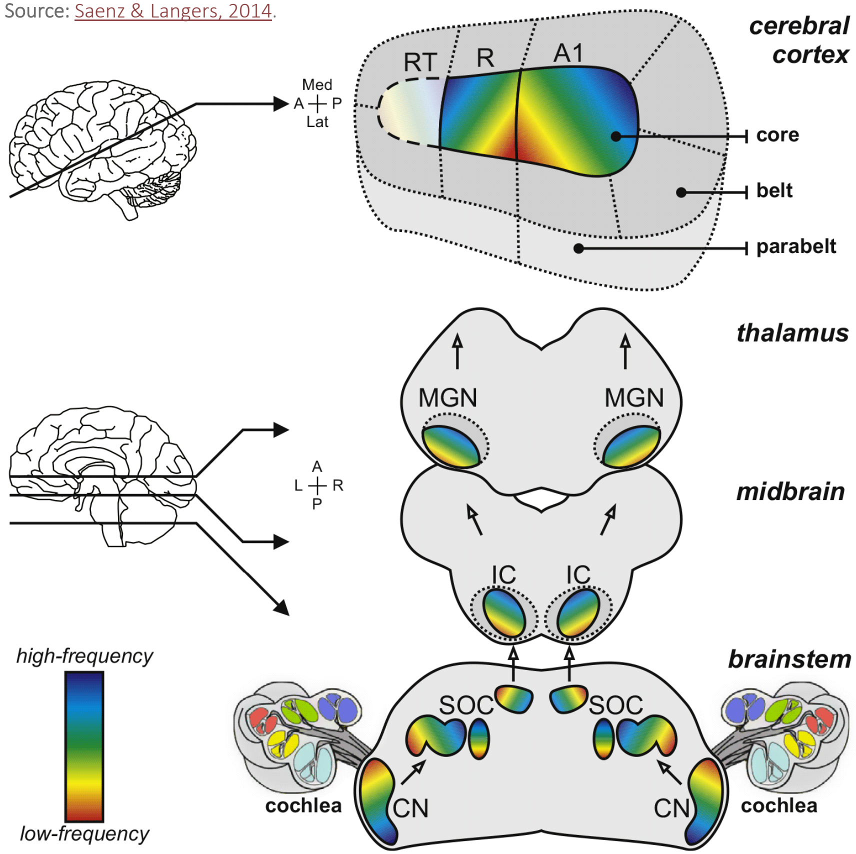
- do mechanoelectrical transduction (convert motion to electricity);
- are the sensory cells in our auditory system.

•• Auditory nervous system: Tonotopy



Source: Tortora & Derrickson: Principles of Anatomy and Physiology, 2016

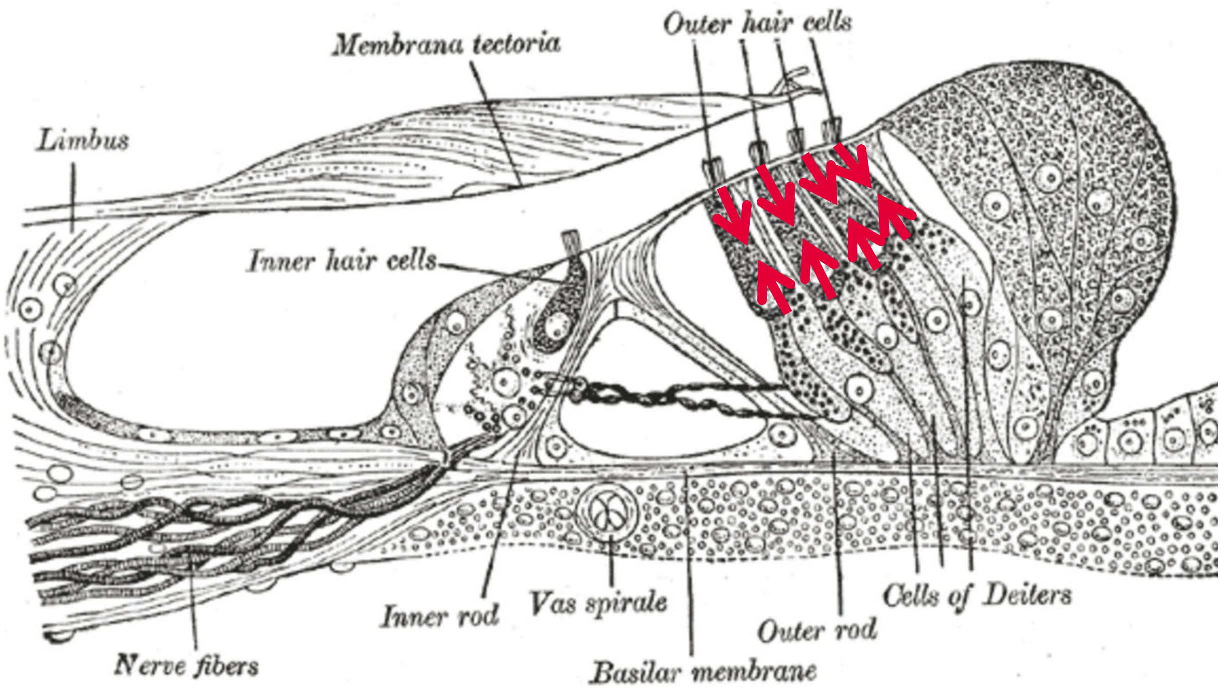
Source: Saenz & Langers, 2014.



Tonotopy is the spatial arrangement of where sounds of different frequencies are processed in the auditory nervous system.

•• Inner ear (cochlea): Cochlear gain

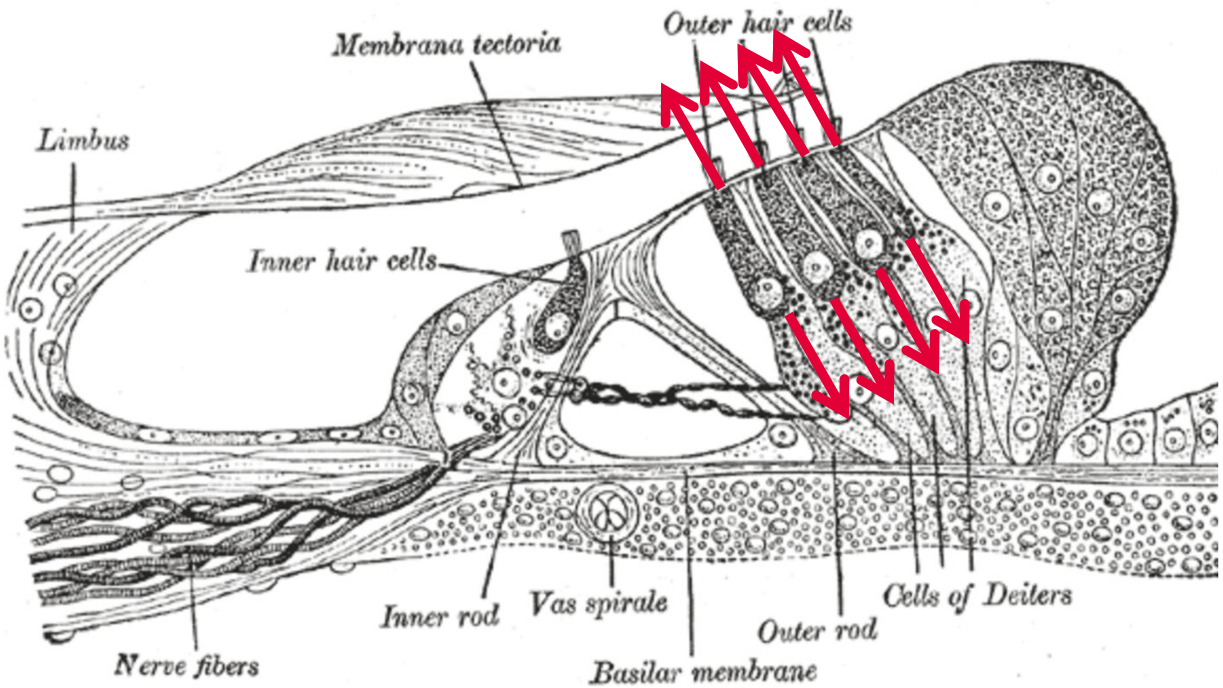
Contraction



audifon hearing systems

•• Inner ear (cochlea): Cochlear gain

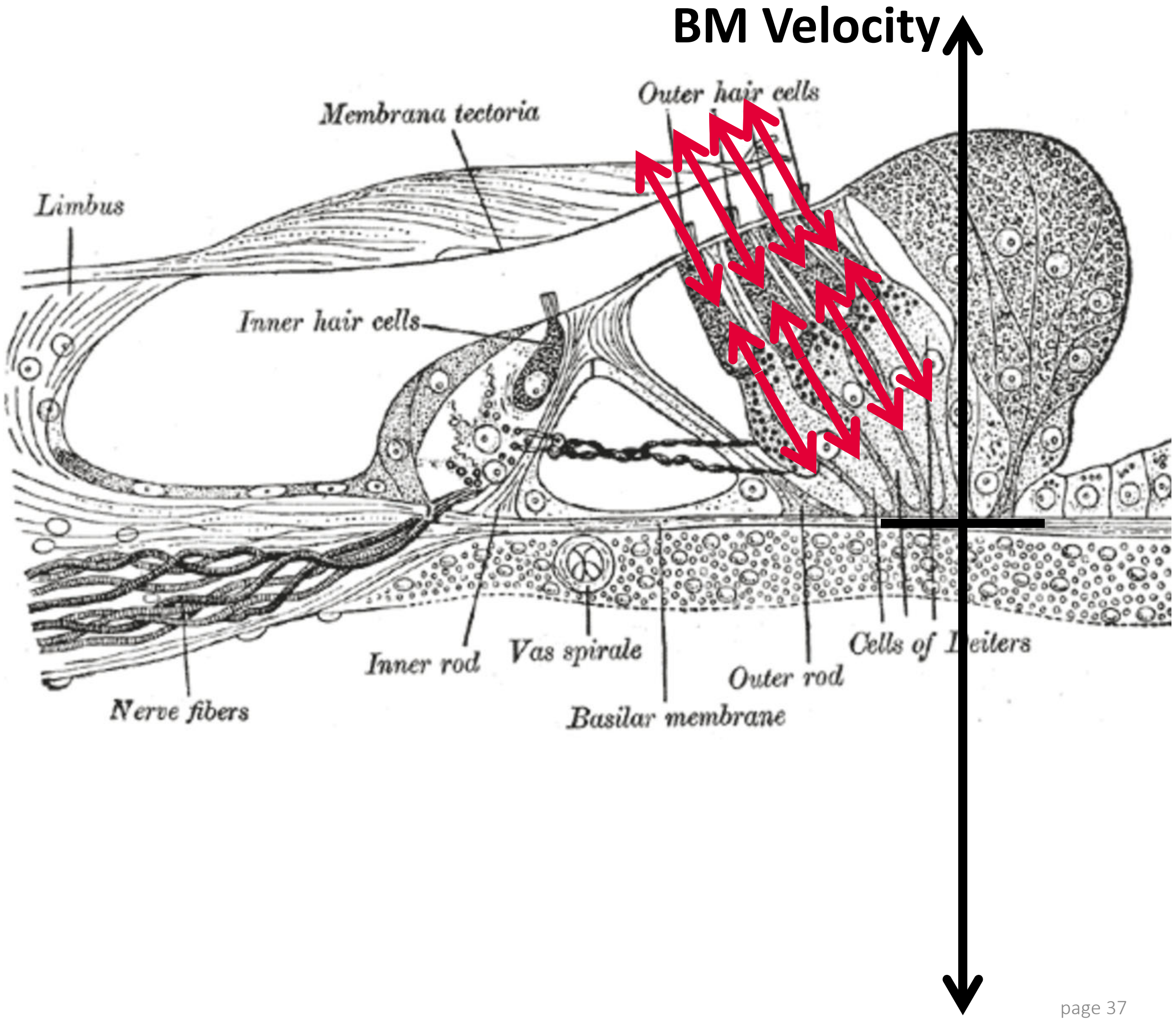
Expansion



audifon
hearing systems

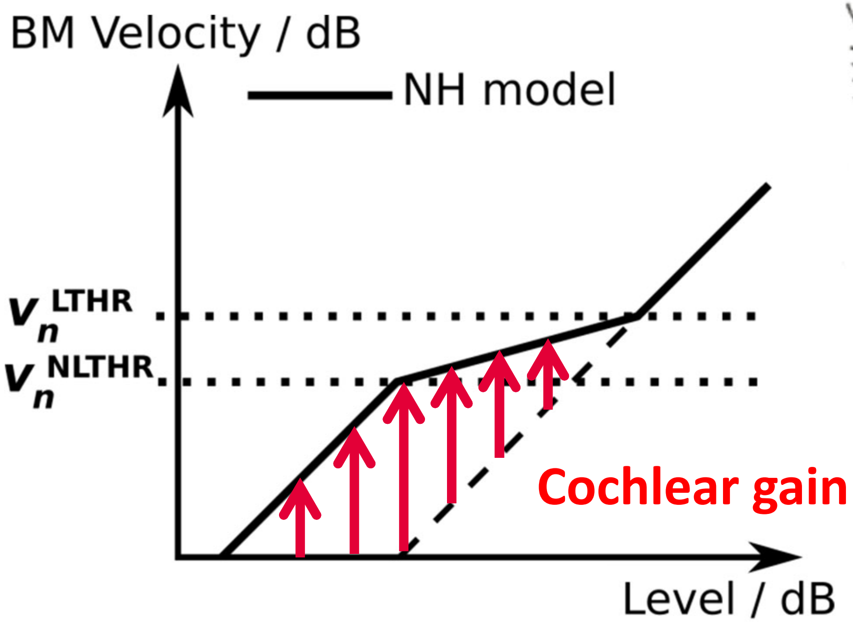
•• Inner ear (cochlea): Cochlear gain

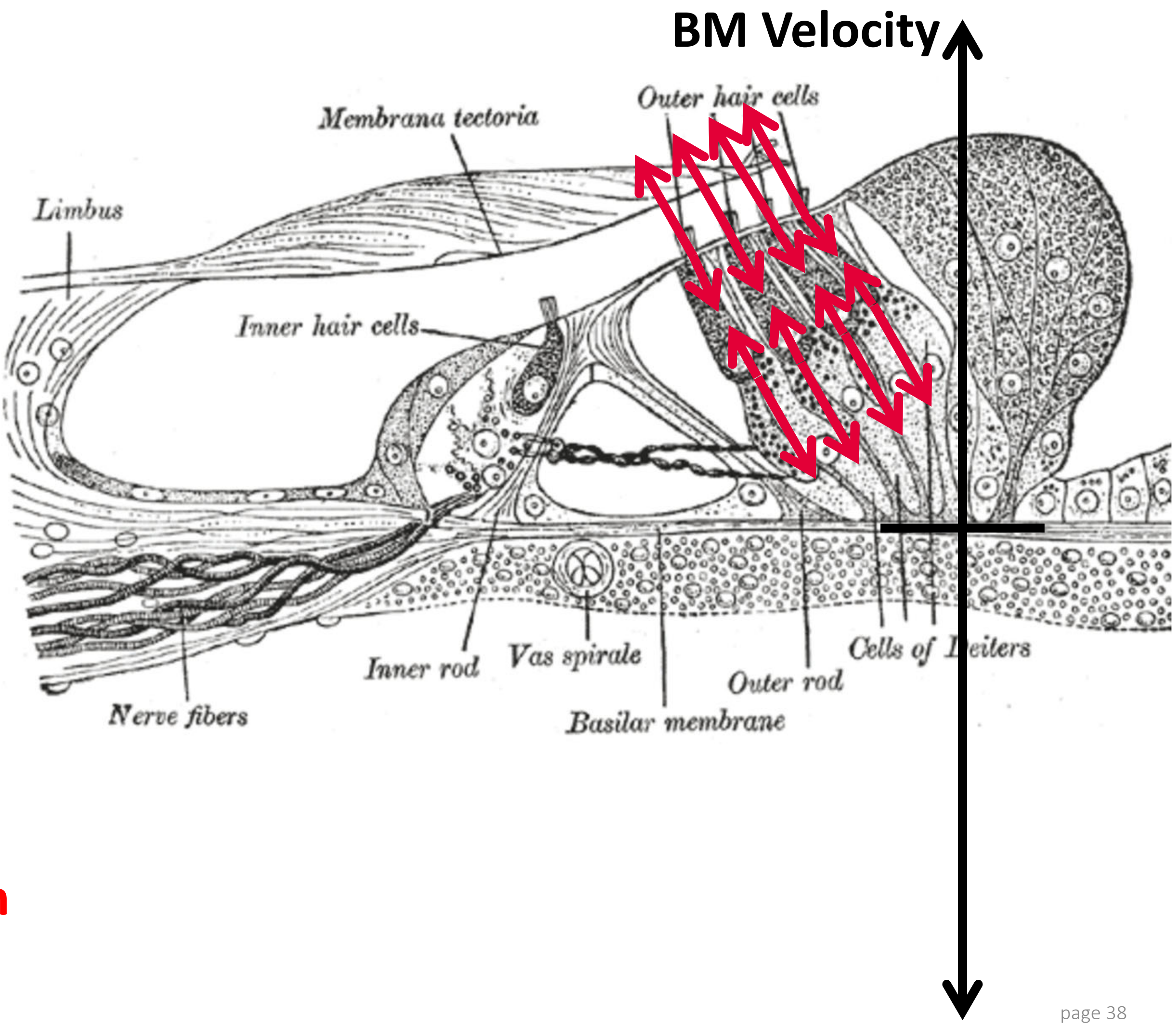
- Outer hair cells (OHC) amplify movements of the basilar membrane (BM)



•• Inner ear (cochlea): Cochlear gain

- Outer hair cells (OHC) amplify movements of the basilar membrane (BM)
- OHC force is limited but mechanical damping force increases with velocity (which increases with level)





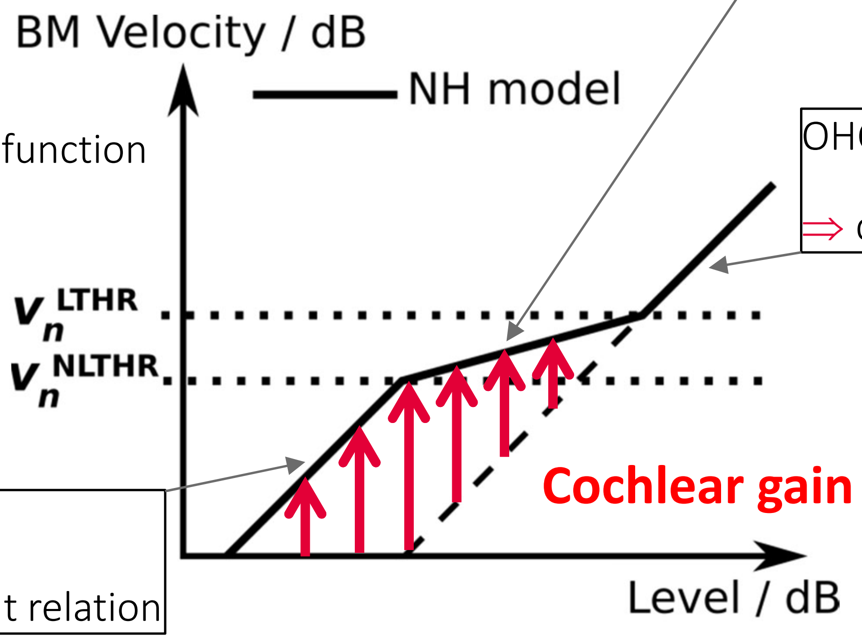
•• Inner ear (cochlea): Cochlear gain

- Outer hair cells (OHC) amplify movements of the basilar membrane (BM)
- OHC force is limited but mechanical damping force increases with velocity (which increases with level)

⇒ “Broken Stick” – input-output function

OHC force ≈ damping force

⇒ compressive input-output relation



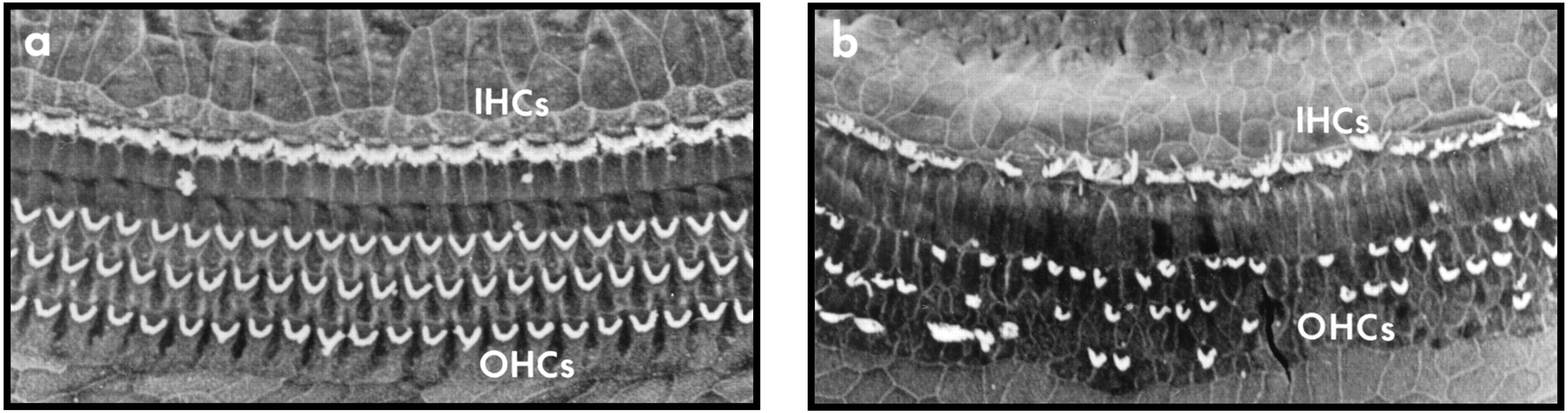
OHC force << damping force

⇒ damped linear input-output relation

OHC force >> damping force

⇒ amplified linear input-output relation

•• Inner ear (cochlea): Sensorineural hearing loss

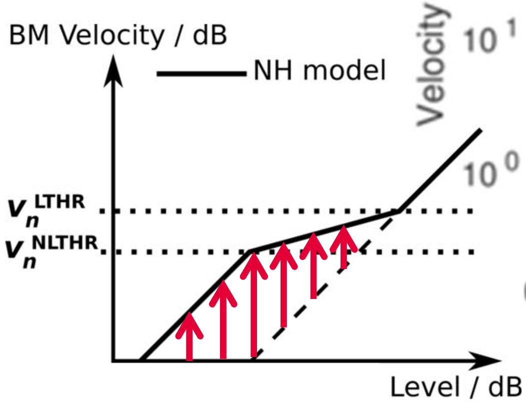


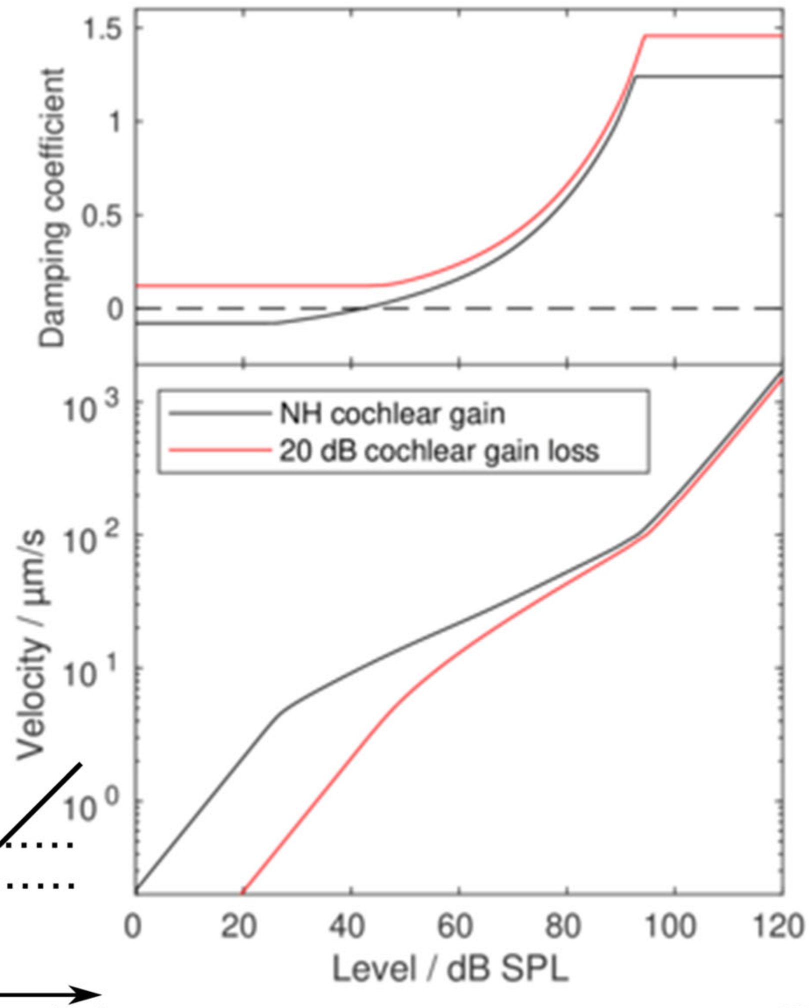
Source: Ryan, 2000

audifon
hearing systems

•• Inner ear (cochlea): Sensorineural hearing loss

- Outer hair cells (OHC) amplify movements of the basilar membrane (BM)
- OHC force is limited but mechanical damping force increases with velocity (which increases with level)
- In models, OHC force and damping force are often combined to a single force with velocity dependent damping coefficient
- Damage to OHCs reduces cochlear gain





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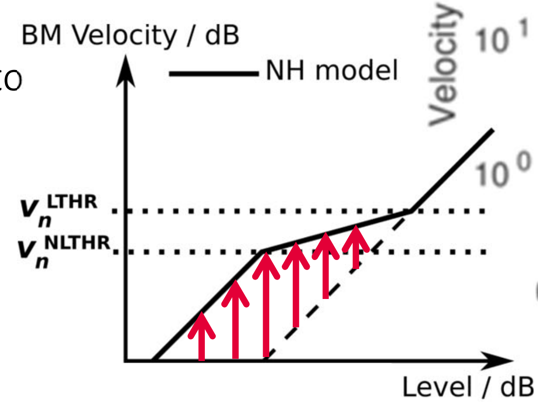
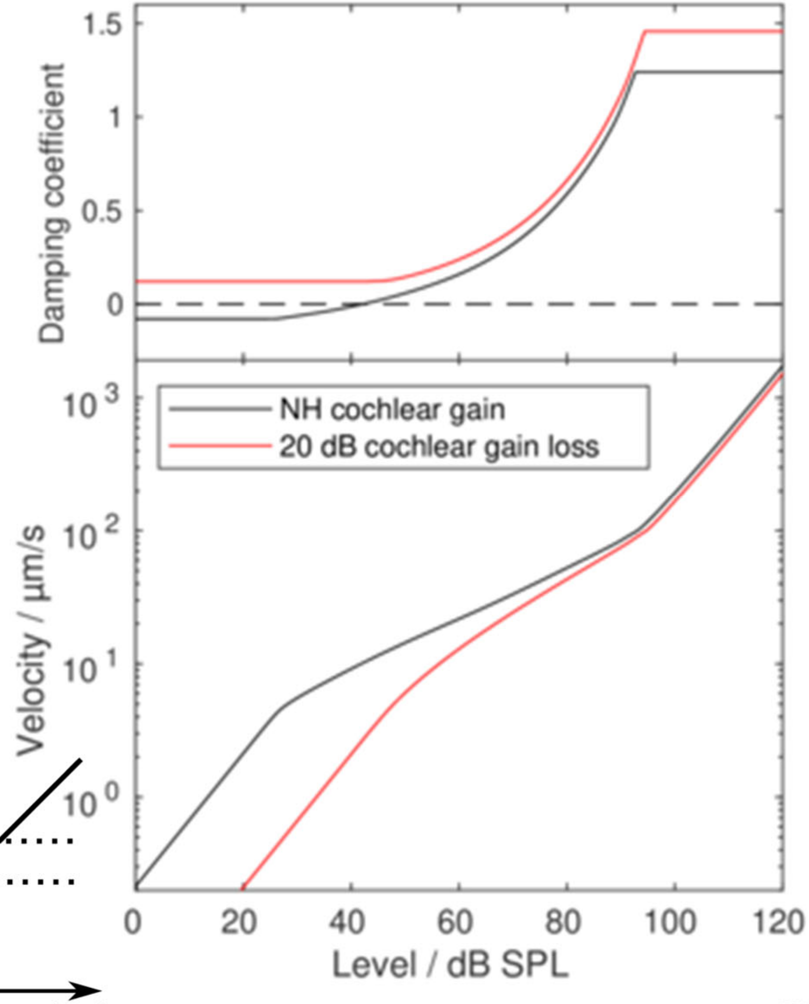
⇒ Higher sound pressure levels required to reach certain BM velocities

⇒ Not much differences at high levels





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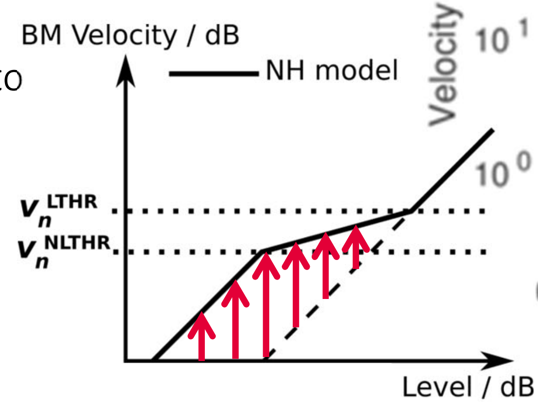
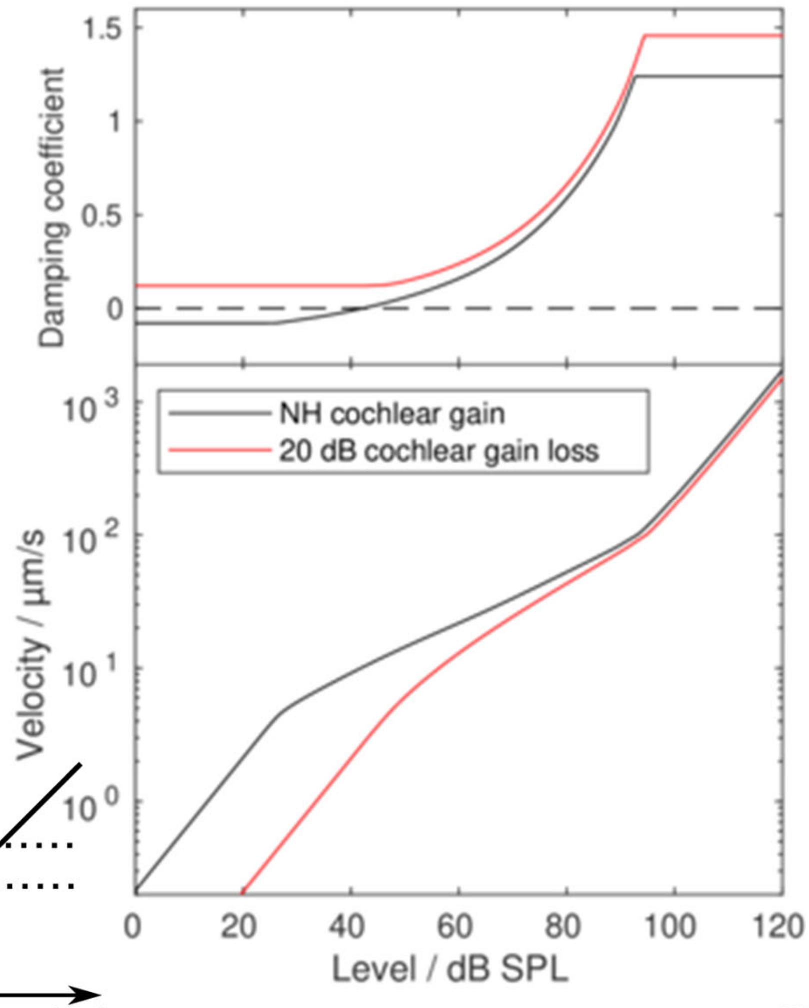
- Damage to OHCs reduces cochlear gain

⇒ Higher sound pressure levels required to reach certain BM velocities

⇒ Not much differences at high levels

⇒ Reduced dynamic range





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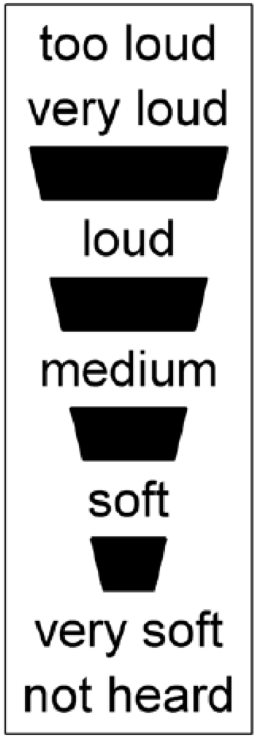
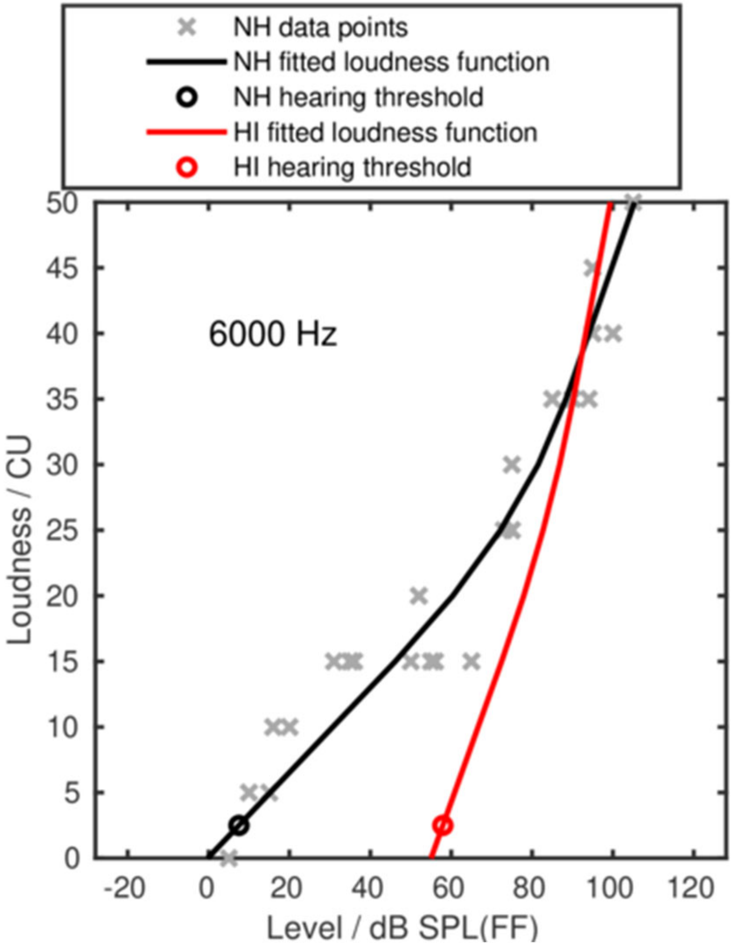
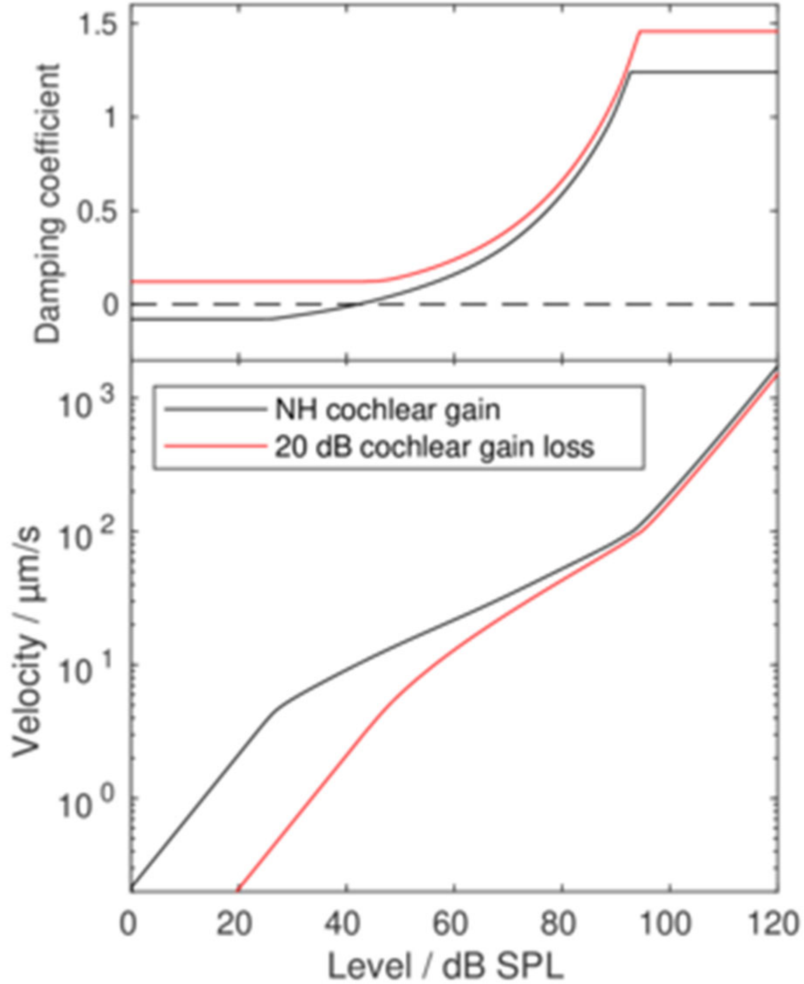




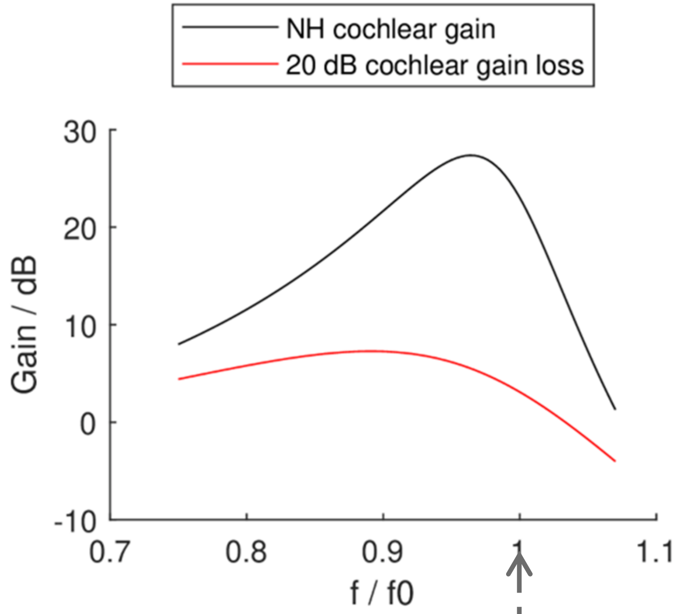


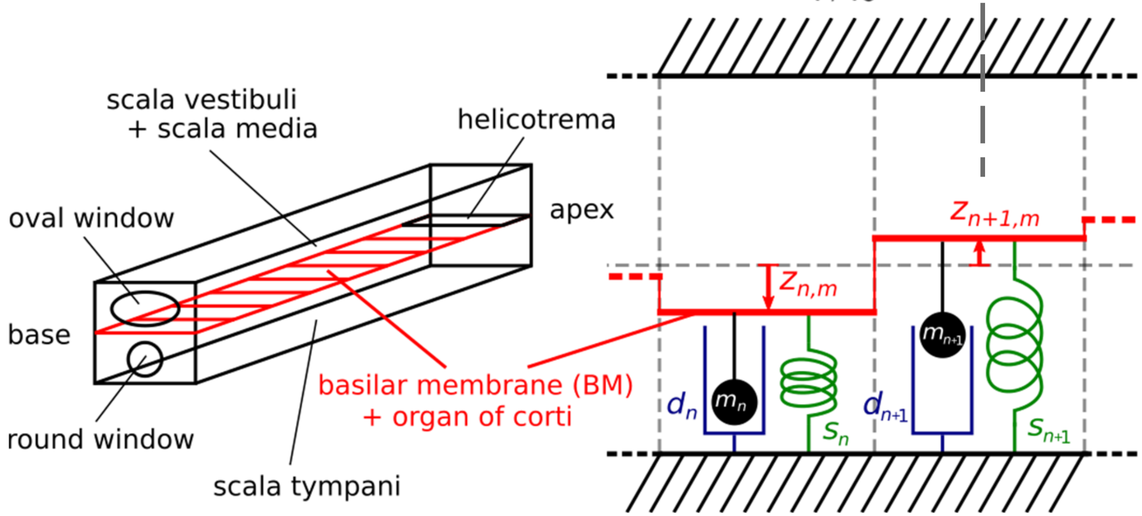
•• Inner ear (cochlea): Frequency discrimination

- Outer hair cells push the basilar membrane

⇒ damping is effectively reduced

⇒ sharper tuning of places to their resonance frequency





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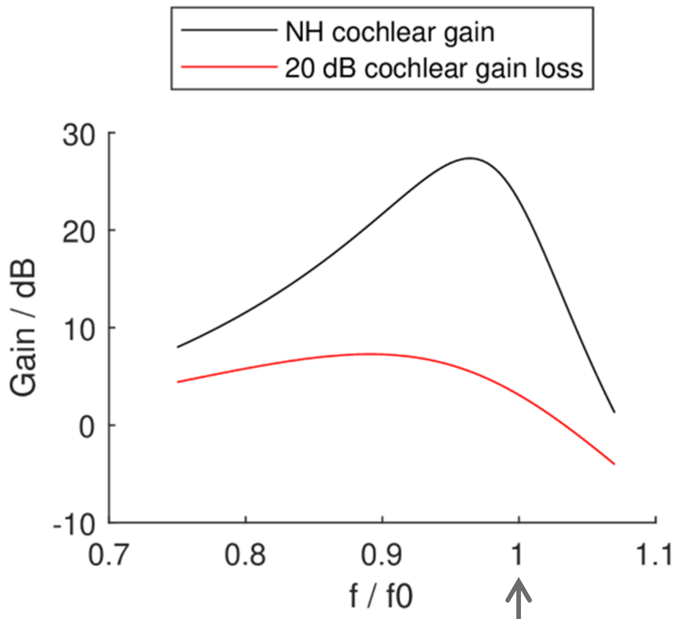

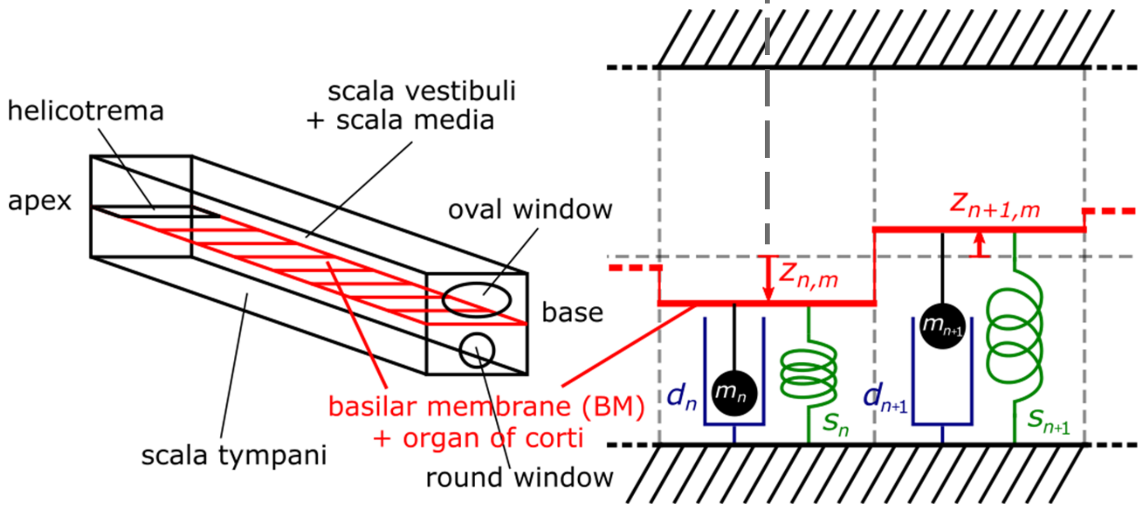

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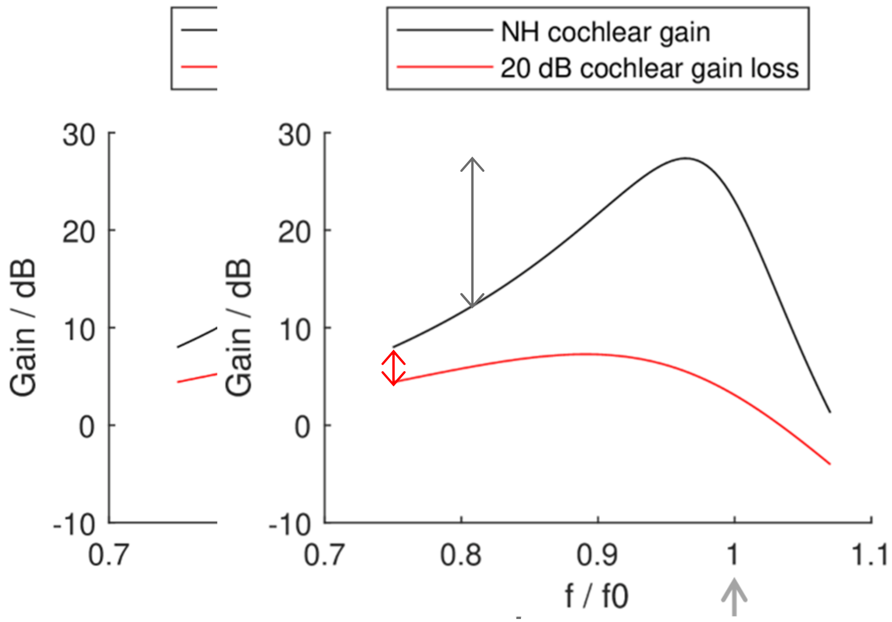
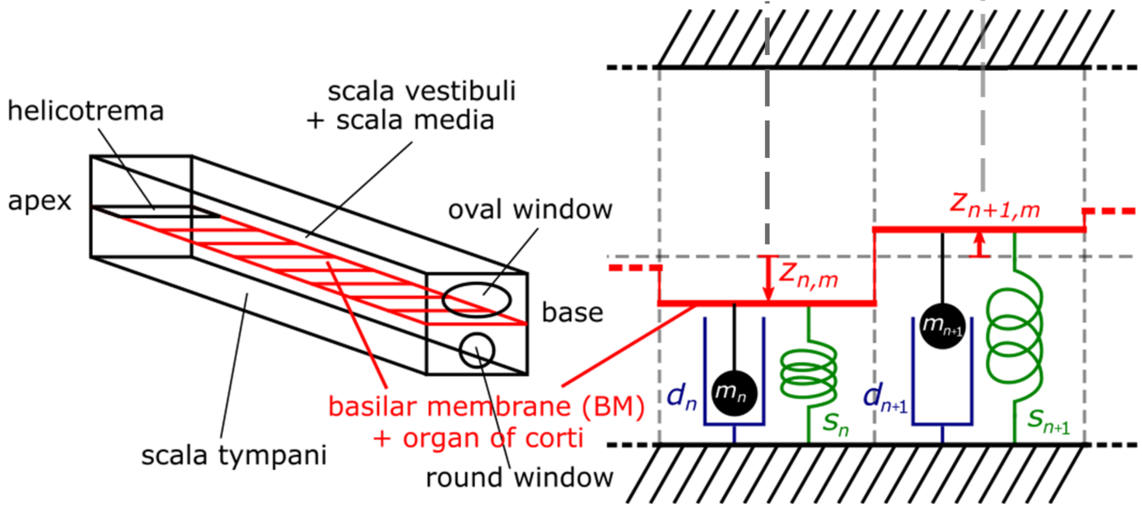




•• Inner ear (cochlea): Frequency discrimination

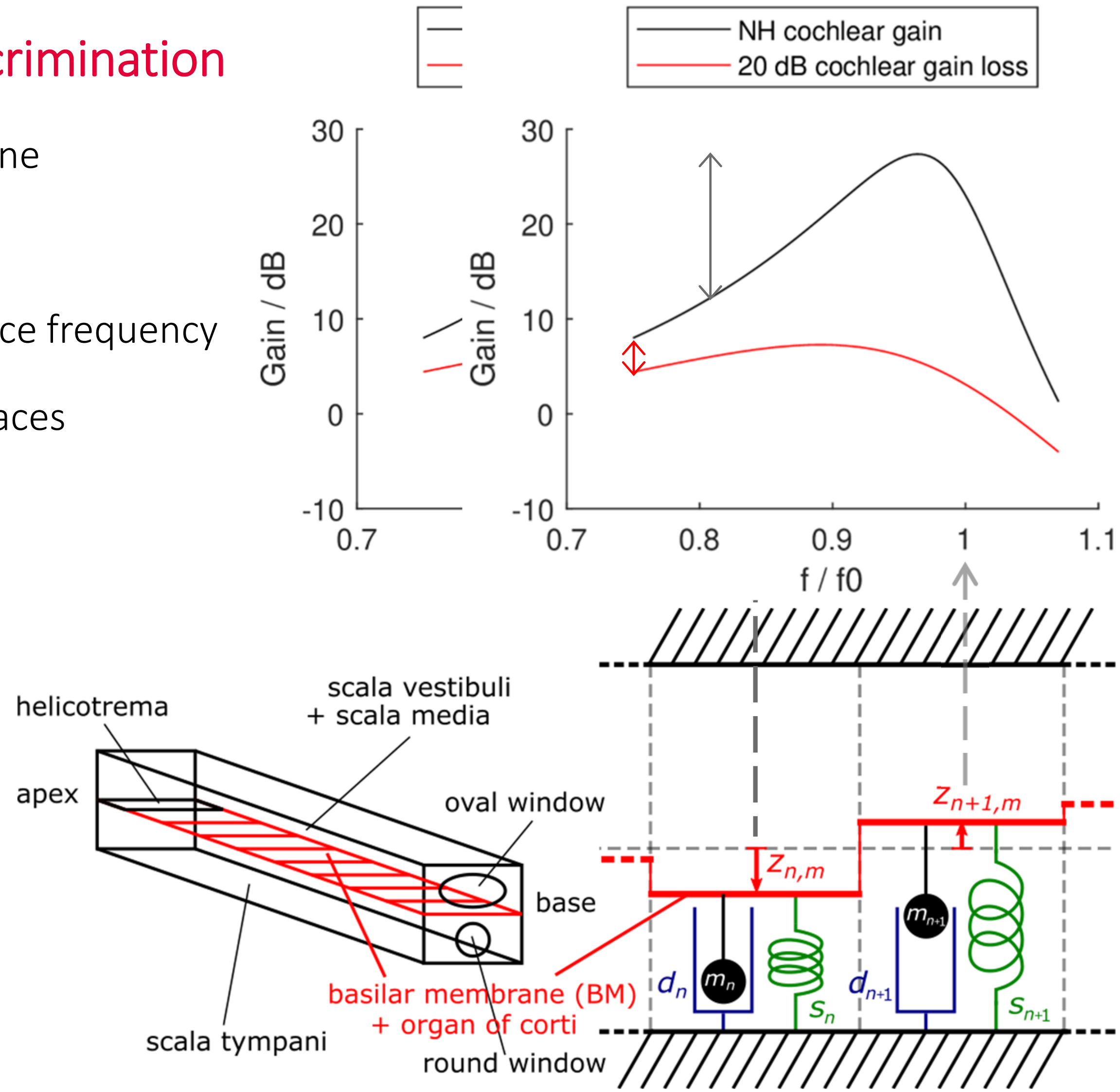
- Outer hair cells push the basilar membrane

⇒ damping is effectively reduced

⇒ sharper tuning of places to their resonance frequency

⇒ higher gain differences at neighboring places
for single frequency components

⇒ better frequency discrimination



•• Inner ear (cochlea): Frequency discrimination

- Outer hair cells push the basilar membrane

⇒ damping is effectively reduced

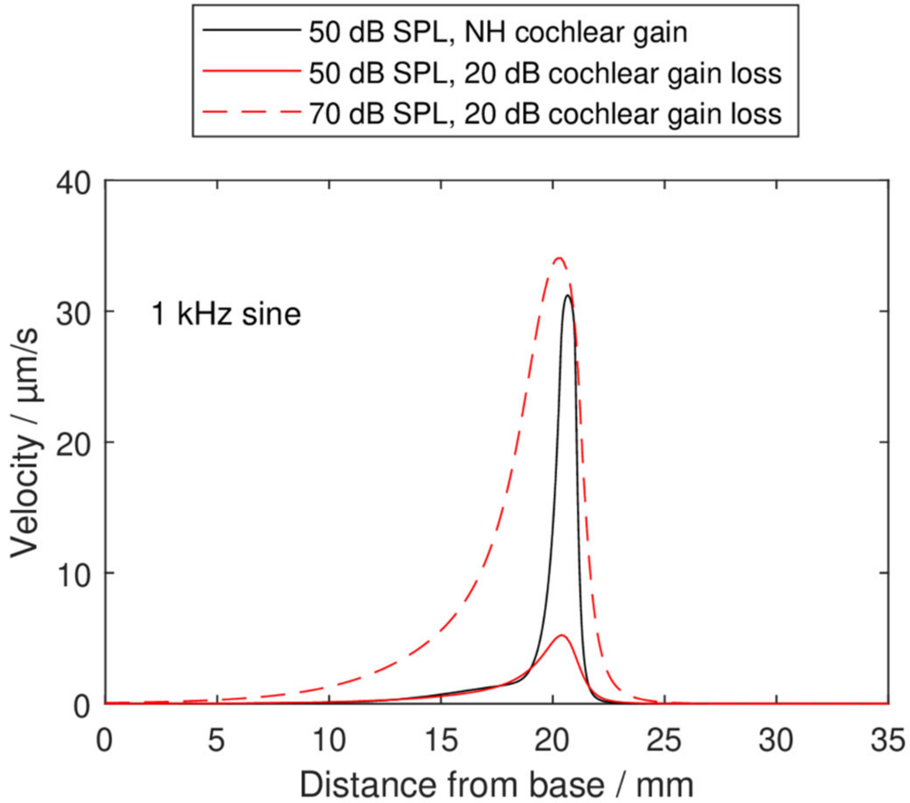
⇒ sharper tuning of places to their resonance frequency

⇒ higher gain differences at neighboring places
for single frequency components

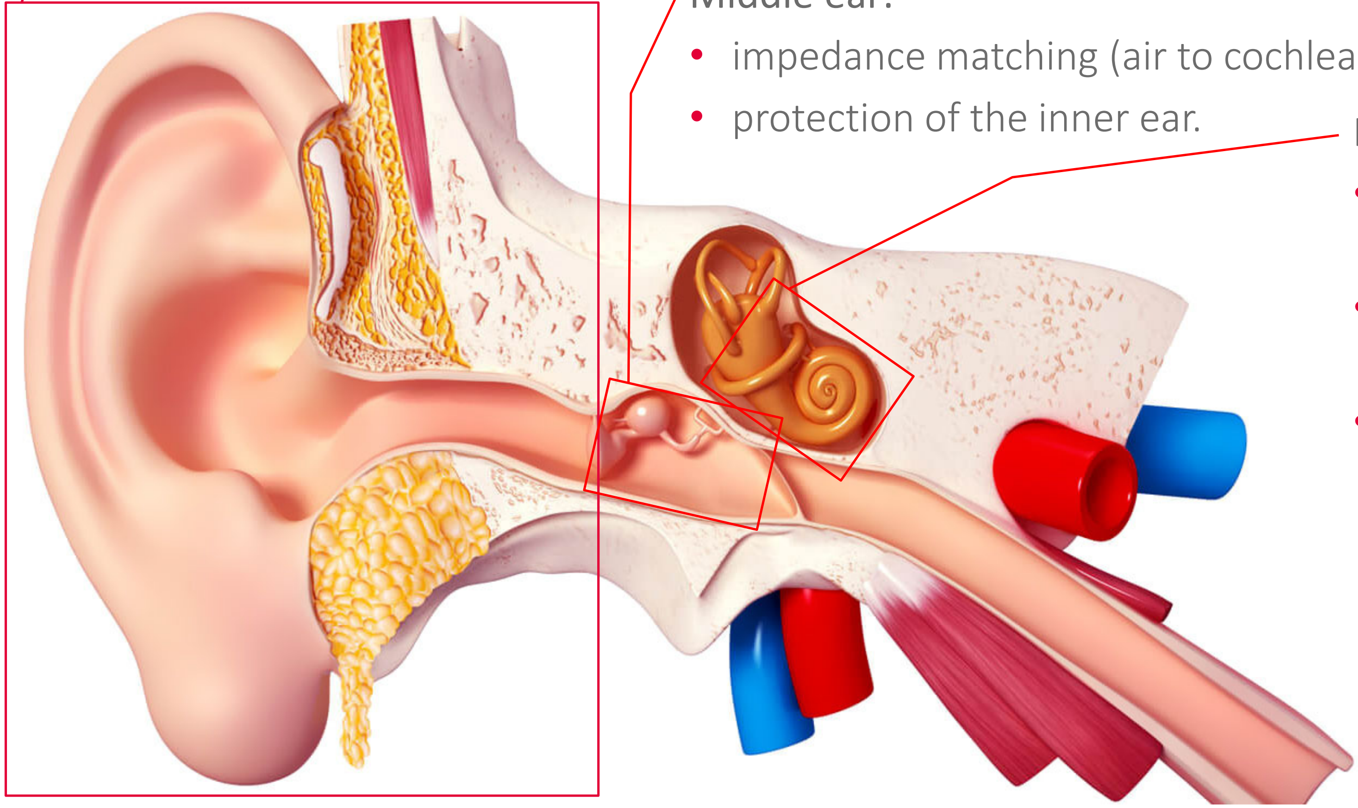
⇒ better frequency discrimination

- Damage to outer hair cells (sensorineural hearing loss)

⇒ worsened frequency discrimination



Short recap



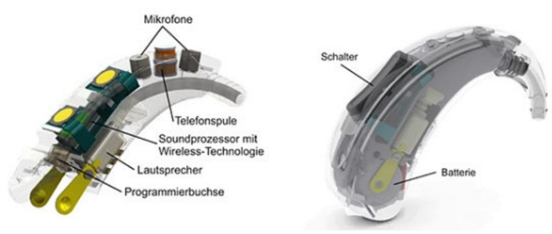
Outer ear: amplification, direction-dependent filtering.

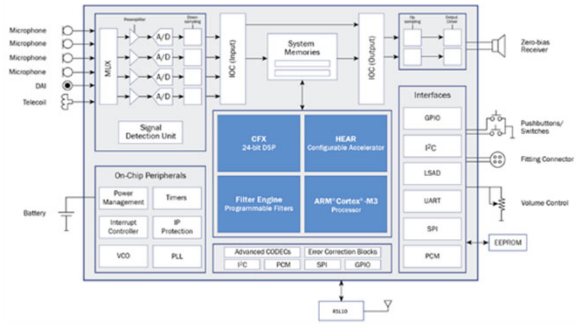
Middle ear:
- impedance matching (air to cochlea),
- protection of the inner ear.

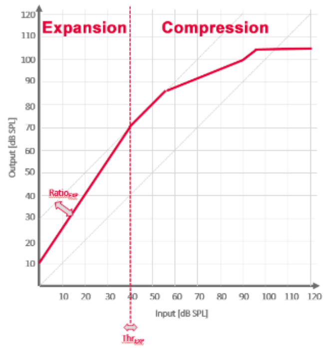
Inner ear (cochlea):
- spectral decomposition of signal (~filter bank),
- extension of dynamic range (compressive nonlinearity),
- transformation into electrical signals.

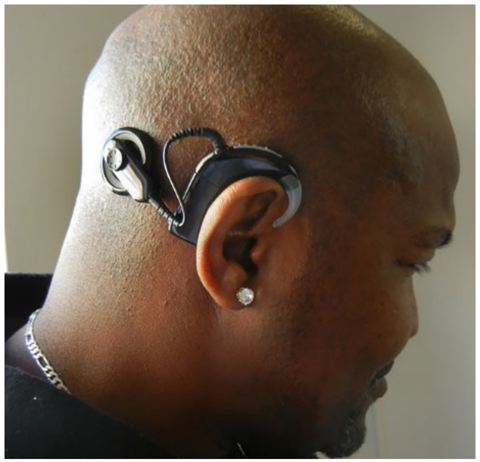
Source: www.lobe.ca, 2021.

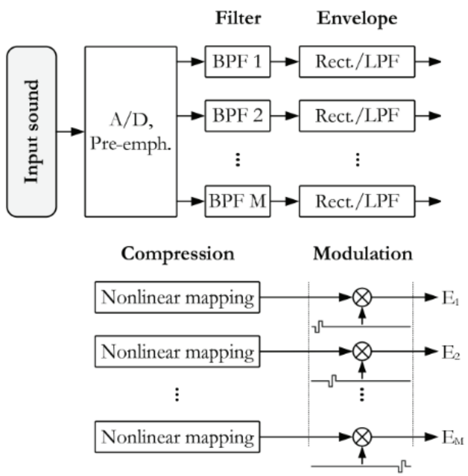
•• Next week

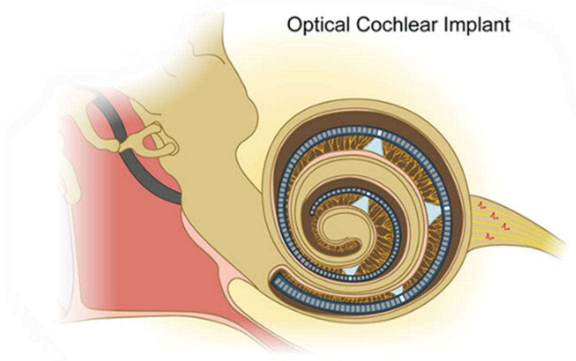

Mikrofone
Telefonspule
Soundprozessor mit Wireless-Technologie
Lautsprecher
Programmierbuchse
Schalter
Batterie


Microphone
Microphone
Microphone
Microphone
DAI
Telecoil
Battery
System Memories
Signal Detection Unit
On-Chip Peripherals
Power Management
Timers
Interrupt Controller
IP Protection
VCO
PLL
CFX 24-bit DSP
HEAR Configurable Accelerator
Filter Engine Programmable Filters
ARM Cortex-M3 Processor
Interfaces
GPIO
LSAD
UART
SPI
PCM
EEPROM
Zero-bias Receiver
Pushbuttons/ Switches
Fitting Connector
Volume Control


Expansion
Compression
Output [dB SPL]
Input [dB SPL]




Filter
Envelope
Input sound
A/D, Pre-emph.
BPF 1
BPF 2
BPF M
Rect./LPF
Rect./LPF
Rect./LPF
Compression
Modulation
Nonlinear mapping
Nonlinear mapping
Nonlinear mapping
E1
E2
EM


Optical Cochlear Implant

audifon hearing systems

Thank you very much!
Questions?

Dr. rer. nat. Iko Pieper
iko.pieper@audifon.com

audifon GmbH & Co. KG