Point-process based representation learning for Electronic Health Records

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Abstract—It is very well accepted that missingness in electronic health records (EHRs) are not at random which is regarded as informative missingness. The clinician's decision on when to observe lab tests over time can be modeled using point processes. We propose a novel framework based on neural point process to analyze laboratory tests of ICU patients. This framework can take into account additional information for better characterization of conditional intensity function (CIF) as well as better accuracy in prediction of future timestamp and labels.

Index Terms— Enter keywords or phrases in alphabetical order, separated by commas. For a list of suggested keywords, send a blank e-mail to keywords@ieee.org or visit the site.

I. INTRODUCTION

Writing an effective abstract is an indispensable part of any form of research, since it that can motivate the audience to read follow the rest of the text. In this task, I have analyzed five abstracts from the field of artificial intelligence (AI). The table in section 2 shows a summary of the most important aspects of the analyzed abstracts.

II. BACKGROUND

Temporal point process Neural temporal point process Handling irregular sampling

III. RELATED WORKS IV. PROPOSED MODEL

The entire data consists of N samples $\mathcal{D} = \{\mathcal{O}_i = (\mathcal{E}_i, \mathcal{S}_i)\}_{i=1}^N$ where \mathcal{E}_i and \mathcal{S}_i represents event and state sequences, respectively.

Each event sequnce consist of L tuples $\mathcal{E}_i = \{(t_j, e_j)\}_{j=1}^{L_i}$ where $t_j \in \mathbb{R}$ is the event timestamp and e_j is the event mark.

This paragraph of the first footnote will contain the date on which you submitted your paper for review. It will also contain support information, including sponsor and financial support acknowledgment. For example, "This work was supported in part by the U.S. Department of Commerce under Grant BS123456."

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Event sequence data consists of N sequences $\{\mathcal{S}_i\}_{i=1}^N$, where each sequence \mathcal{S}_i is a series of L_i events $\{(t_j,e_j)\}_{j=1}^{L_i}$. Here, e_j represents events that could be independent our mutually exclusive occurring at t_i .

In addition to the event data, we might have additional information $\{\mathcal{D}_i\}_{i=1}^N$. Suppose that each state is represented as $\{(t_k,v_k,m_k)\}_{k=1}^N$, consisting of a time value $t_k\in\mathbb{R}^+$, an observed value $z_k\in\mathbb{R}$ and a modality indicator $m_k\in\{1,...,M\}$.

General schematic of TEDAM is depicted in FIG which consists of two separate module: Transformer Event Encoder (TEE) and Deep Attention Module (DAM). TEE encodes timestamp and mark of events using a transformer architecture, while DAM encodes all available information using one-dimensional attention mechanism. Finally, the learned representations are concatenated to be optimized for different loss functions.

A. Event Encoder

We use a similar transformer architecture [thp] for encoding events with minor modifications. A transformer architecture is capable of .

let , that can be embedded using a trainable embedding matrix.

In the first step, we embed all event marks $E_{emb} = E \times U$ where $E_i \in [L,K]$ is the binary encoding matrix of all event marks (multi-label or multi-class), and $W_{emb} \in \mathbb{R}^{K \times d_{emb}}$ is the trainable embedding matrix. In the second step, timestamps should be encoded and added to the event embedding, however, we propose to concatenate time encodings that can lead to better characterization of conditional intensity functions. Finally, the input of the transformer encoder will be $x_{emb} = [y(k_j), z(t_j)]$.

Here, we use the standard transformer encoder similar to [vaswani] with masking matrix to prevent the model from looking into the future. we obtain the encoded matrix $H = (h_1, ..., h_j, ..., h_L)$ where h_j containes the all available information before occurrence of j - th event.

B. bin of Event Encoder

it is necessary to include temporal information. Similar to the original positional encoding [vaswani], we use a temporal encoding procedure:

$$[z(t_j)]_k = \begin{cases} \sin\left(\frac{t_j}{\mathcal{T}^{(k-1)/d_t}}\right) & \text{if } k \text{ is odd} \\ \sin\left(\frac{t_j}{\mathcal{T}^{k/d_t}}\right) & \text{if } k \text{ is even} \end{cases}$$
(1)

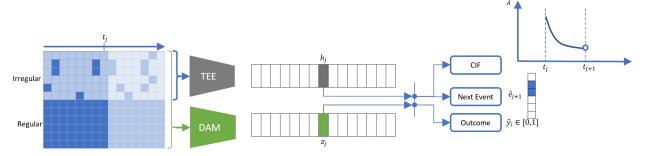


Fig. 1. Magnetization as a function of applied field. It is good practice to explain the significance of the figure in the caption.

Here, $d_t \in \mathbb{N}$ is the dimensionality of encoded timestamp and $z \in \mathbb{R}^{d_t}$ is the embeding vector of timestamp.

Each event mark e_j is projected to a sparse binary vector representation. We add an embedding layer to achieve a more compact and efficient representation emb. Here, w and b are weights and biases of the embedding layer which can be learned during network training.

While previous works suggested adding temporal encoding to the embedded events, we propose to concatenate these two vectors. The effectiveness of this concatenation is further investigated in the results.

$$x_{emb} = [y(k_j), z(t_j)] \tag{2}$$

Now that the x_{emb} is ready for encoding, it is encoded through a standard transformer encoder with multiple layers and attention heads.

$$x_{enc} = TE(x_{emb}) \tag{3}$$

C. State Encoder

Here, we propose a method to incorporate additional information for a better representation. In healthcare, much data is available from different modalities such as vital signs and laboratory values.

Similar to [setF], we use an attention-based aggregation approach for encoding all additional information. Each side information (t_k, v_k, m_k) can be represented by $s_k = (z(t_k), v_k, m_k)$, we define attention $a(S_k, s_k)$

We define S_p to be the set of the first p available information. The goal is to calculate $a(S_p,s_k), k \leq p$ that is the relevance of k-th observation s_k to the first p observed values S_p . This is achieved by computing an embedding of the set elements using a smaller set functions f', and projecting the concatenation of the set representation and the individual set element into d-dimensional space:

$$f'(S_p) = g'\left(\frac{1}{p} \sum_{s_k \in S_p} h'_{\theta}(s_k)\right)$$
$$K_p = [f'(S_p), s_p]^T W^K$$

Furthermore, we define a query vector $w^q \in \mathbb{R}^d$, which allows the model to summarize different aspects of the dataset via

$$e_p = \frac{K_p.w^q}{\sqrt{d}}$$

Now, the desired attention can be computed as follows:

$$a(\mathcal{S}_p, s_k) = \frac{\exp(e_p)}{\sum_{k \le p} \exp(e_k)}$$

Finally, we compute a weighted aggregation of set elements:

$$f(\mathcal{S}_p) = g_{\psi} \left(\sum_{s_k \in \mathcal{S}_p} a(\mathcal{S}_p, s_k) h_{\theta}(s_k) \right)$$

Without loss of generality, we can consider multiple heads by adding an additional dimension to keys and queries.

All formulas are:

$$\begin{cases} f'(\mathcal{S}_p) = g'\left(\frac{1}{p}\sum_{s_k \in \mathcal{S}_p} h'_{\theta}(s_k)\right) \\ K_p = [f'(\mathcal{S}_p), s_p]^T W^K \\ e_p = \frac{K_p.w^q}{\sqrt{d}} \\ a(\mathcal{S}_p, s_k) = \frac{\exp(e_p)}{\sum_{k \le p} \exp(e_k)} \\ f(\mathcal{S}_p) = \sum_{s_k \in \mathcal{S}_p} a(\mathcal{S}_p, s_k) h_{\theta}(s_k) \\ z_p = g_{\psi}\left(f(\mathcal{S}_p)\right) \end{cases}$$

D. Mark and Time Decoder

by concatenating encoded events x_{enc} and additional information $f'(S_p)$, we can predict next marks and times as follows:

$$\hat{e}_{j+1} = MLP([x_j, f'(\mathcal{S}_j)]) \tag{4}$$

$$\hat{t}_{j+1} = MLP([x_j, f'(\mathcal{S}_j)]) \tag{5}$$

$$\mathcal{L}_{mark} = \tag{6}$$

$$\mathcal{L}_{time} = \sum_{j=1}^{L-1} \left((\hat{t}_{j+1} - t_j) - (t_{j+1} - t_j) \right)^2 \tag{7}$$

E. Event Decoder

Once we obtain a representation of a patient using embedded events and states, we can try to parameterize conditional intensity functions (CIFs) of the events.

In neural point process literature, many approaches have been propose to decode either conditional or cumulative intensity function.

$$\lambda_k(t|\mathcal{H}_t) = f_k \left(\alpha_k \frac{t - t_j}{t_j} + \mathbf{w}_k^T \mathbf{x}_{enc}(t_j) + \mathbf{y}_k^T \mathbf{s}_{enc}(t_j) + b_k \right)$$
(8)

$$\lambda_k(t|\mathcal{H}_t) = f_k \left(\alpha_k \frac{t - t_j}{t_j} + \mathbf{w}_k^T \mathbf{x}_{enc}(t_j) + b_k \right)$$
(9)

V. EXPERIMENTS

Datasets

Physionet 2019 Sepsis Early Prediction Challenge (P19).

This dataset contains clinical data of about 40k patients in ICU. Clinical data consist of demographics, vital signs and laboratory values as well as sepsis label in a one-hour time grid. Our objective is to predict the timestamp of next lab sampling events as well as measured variables (event marks) given the patient history.

MIMIC-IV (*M4*). We selected Medical Information Mart for Intensive Care (MIMIC) IV [1], which is a real-world clinical database comprising health data relating to over 40,000 patients admitted to ICU at the Beth Israel Deaconess Medical Center.

Synthea(*Syn*). We used the Synthea simulator (Walonoski et al., 2018) which generates patient-level EHRs using human expert curated Markov processes. Here, we reused the already processed version of this data by Edgauard.

Stackoverflow (SO). StackOverflow is a question-answering website. The website rewards users with badges to promote engagement in the community, and the same badge can be rewarded multiple times to the same user. We collect data in a two-year period, and we treat each user's reward history as a sequence. Each event in the sequence signifies receipt of a particular medal.

Scenarios

To investigate the effectiveness of the proposed method, we consider three input scenarios (TE, DA, TE+DA) as well as three loss functions (next event, CIF, next event+CIF) which would result in nine scenarios.

The first series of experiments are conducted to investigate the advantage of encoding additional information for paramterization of intensity functions. We consider seven scenarios: Here, the baseline models

To show the effectiveness of time concatenation we report.

Baselines

we use NEURALTPP that is already developed pipeline by as they already considered a lot of comibinations.

Metrics

We report the weighted AUPRC, AUROC of next predicted event as well as root mean square error (RMSE) of next measurement interval. For evaluating the goodness of fit for the parameterized point process, we report normalized negative likelihood normalized by number of ocurred event (NLL/events). Furthermore, we can also evaluate the learned representation of each patient to predict the sepsis label in a binary classification task.

VI. RESULTS AND DISCUSSION

In this section, we present our results regarding the advantage of state and event encoding.

A. Effect of minor improvements

effect of time concatenation compare single+mark with mc or ml

TABLE I ADD CAPTION

		shp+		
Dataset	Metric	concat	sum	baseline
SO	NLL	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	AUROC	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	time	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
Synthea	NLL	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	AUROC	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	time	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
ReTweet	NLL	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	AUROC	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	time	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)

B. Negative Likelihood with state encoding

Table 1 shows the result for estimation of negative likelihood in different datasets and scnearios. It is obvious that state encoding has led to lower NLL.

TABLE II
ADD CAPTION

		Model		
Dataset	setting	TE	TE+DAM	TE+noise
P12	sc	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
p19	sc	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)

can u provide one example patient?

C. Downstream task with event encoding

Another key element of our work is to show the effectiveness of point process modeling for a down-stream task. In Table, we have reported the performance metrics for the mortality prediction task. We have compared our results with several sota's DL models that are compatible with irregular time series.

TABLE III **ADD CAPTION**

			F1		AUPRC		AUROC	
Dataset	Setting	Center	DAM	TE+DAM	DAM	TE+DAM	DAM	TE+DAM
-		1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	sc	2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
		3	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
		1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
P12	mc1	2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
mo		3	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc2	-	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	seft	-	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
		1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	sc	2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
		3	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
P19 _		1	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc1	2	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
		3	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	mc2	-	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)
	seft	-	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)	0.55 (0.02)

D. Learned representions

Fig 1 visualizes the tsne plot for the two scenarios.

E. Model interpretability

one advantage of proposed method is use of attention mechanisms in both event and state encoder. Fig 1 shows the attention mechanism

F. Likelihood estimation

Although CIF does not improve mark prediction, it has led to better representation of patient for downstream task such as sepsis prediction.

In addition, we can interpret some of learned CIF patterns. explain the effect of time concatenation in SO dataset tsne of learned representation. 4 modes:

• (DA,TE)-¿(Mark, CIF) attention of DA for sepsis prediction attention matrix of events for SO dataset

VII. CONCLUSION VIII. INTRODUCTION

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Define abbreviations and acronyms the first time they are used in the text, even after they have already been defined in the abstract. Abbreviations such as IEEE, SI, ac, and dc do not have to be defined. Abbreviations that incorporate periods should not have spaces: write "C.N.R.S.," not "C. N. R. S." Do not use abbreviations in the title unless they are unavoidable (for example, "IEEE" in the title of this article).

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Use a zero before decimal points: "0.25," not ".25." Use "cm 3 ," not "cc." Indicate sample dimensions as "0.1 cm \times 0.2 cm," not " 0.1×0.2 cm²." The abbreviation for "seconds" is "s," not "sec." Use "Wb/m2" or "webers per square meter," not "webers/m2." When expressing a range of values, write "7 to 9" or "7–9," not "7~9."

A parenthetical statement at the end of a sentence is punctuated outside of the closing parenthesis (like this). (A parenthetical sentence is punctuated within the parentheses.) In American English, periods and commas are within quotation marks, like "this period." Other punctuation is "outside"! Avoid contractions; for example, write "do not" instead of "don't." The serial comma is preferred: "A, B, and C" instead of "A, B and C."

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$$E = mc^2. (10)$$

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Use either SI (MKS) or CGS as primary units. (SI units are strongly encouraged.) English units may be used as secondary units (in parentheses). This applies to papers in data storage. For example, write "15 Gb/cm² (100 Gb/in²)." An exception is when English units are used as identifiers in trade, such as "3½-in disk drive." Avoid combining SI and CGS units, such as current in amperes and magnetic field in oersteds. This often leads to confusion because equations do not balance dimensionally. If you must use mixed units, clearly state the units for each quantity in an equation.

The SI unit for magnetic field strength H is A/m. However, if you wish to use units of T, either refer to magnetic flux density B or magnetic field strength symbolized as $\mu_0 H$. Use the center dot to separate compound units, e.g., "A·m²."

X. SOME COMMON MISTAKES

The word "data" is plural, not singular. The subscript for the permeability of vacuum μ_0 is zero, not a lowercase letter "o." The term for residual magnetization is "remanence"; the adjective is "remanent"; do not write "remnance" or "remnant." Use the word "micrometer" instead of "micron." A graph within a graph is an "inset," not an "insert." The word "alternatively" is preferred to the word "alternately" (unless you really mean something that alternates). Use the word "whereas" instead of "while" (unless you are referring to simultaneous events). Do not use the word "essentially" to mean "approximately" or "effectively." Do not use the word "issue" as a euphemism for "problem." When compositions are not specified, separate chemical symbols by en-dashes; for example, "NiMn" indicates the intermetallic compound Ni_{0.5}Mn_{0.5} whereas "Ni-Mn" indicates an alloy of some composition Ni_xMn_{1-x} .

Be aware of the different meanings of the homophones "affect" (usually a verb) and "effect" (usually a noun), "complement" and "compliment," "discreet" and "discrete," "principal" (e.g., "principal investigator") and "principle" (e.g., "principle of measurement"). Do not confuse "imply" and "infer."

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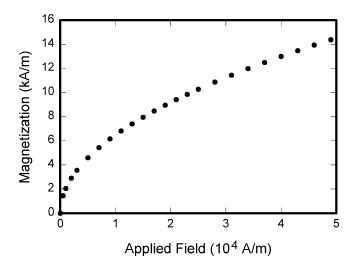


Fig. 2. Magnetization as a function of applied field. It is good practice to explain the significance of the figure in the caption.

XI. GUIDELINES FOR GRAPHICS PREPARATION AND SUBMISSION

A. Types of Graphics

The following list outlines the different types of graphics published in IEEE journals. They are categorized based on their construction, and use of color/shades of gray:

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TABLE IV
UNITS FOR MAGNETIC PROPERTIES

Symbol	Quantity	Conversion from Gaussian and
-		CGS EMU to SI a
Φ	magnetic flux	$1 \text{ Mx} \rightarrow 10^{-8} \text{ Wb} = 10^{-8} \text{ V} \cdot \text{s}$
B	magnetic flux density,	$1 \text{ G} \rightarrow 10^{-4} \text{ T} = 10^{-4} \text{ Wb/m}^2$
	magnetic induction	
H	magnetic field strength	1 Oe $\to 10^3/(4\pi)$ A/m
m	magnetic moment	1 erg/G = 1 emu
		$\rightarrow 10^{-3} \text{ A} \cdot \text{m}^2 = 10^{-3} \text{ J/T}$
M	magnetization	$1 \text{ erg/}(G \cdot \text{cm}^3) = 1 \text{ emu/cm}^3$
		$\rightarrow 10^3 \text{ A/m}$
$4\pi M$	magnetization	$1 \text{ G} \to 10^3/(4\pi) \text{ A/m}$
σ	specific magnetization	$1 \operatorname{erg}/(G \cdot g) = 1 \operatorname{emu/g} \rightarrow 1$
		A·m ² /kg
j	magnetic dipole	1 erg/G = 1 emu
	moment	$\rightarrow 4\pi \times 10^{-10} \text{ Wb·m}$
J	magnetic polarization	$1 \operatorname{erg/(G \cdot cm^3)} = 1 \operatorname{emu/cm^3}$
		$\rightarrow 4\pi \times 10^{-4} \text{ T}$
χ, κ	susceptibility	$1 \rightarrow 4\pi$
$\chi_{ ho}$	mass susceptibility	$1 \text{ cm}^3/\text{g} \to 4\pi \times 10^{-3} \text{ m}^3/\text{kg}$
μ	permeability	$1 \rightarrow 4\pi \times 10^{-7} \text{ H/m}$
		$= 4\pi \times 10^{-7} \text{ Wb/(A·m)}$
μ_r	relative permeability	$\mu \to \mu_r$
w, W	energy density	$1 \text{ erg/cm}^3 \rightarrow 10^{-1} \text{ J/m}^3$
N, D	demagnetizing factor	$1 \rightarrow 1/(4\pi)$

Vertical lines are optional in tables. Statements that serve as captions for the entire table do not need footnote letters.

^aGaussian units are the same as cg emu for magnetostatics; Mx = maxwell, G = gauss, Oe = Oersted; Ce = We = Oersted; Ce = Ve = Oersted; Ce = Oersted; Ce

D. Sizing of Graphics

Most charts, graphs, and tables are one column wide (3.5 inches/88 millimeters/21 picas) or page wide (7.16 inches/181 millimeters/43 picas). The maximum depth a graphic can be is 8.5 inches (216 millimeters/54 picas). When choosing the depth of a graphic, please allow space for a caption. Figures can be sized between column and page widths if the author chooses, however it is recommended that figures are not sized less than column width unless when necessary.

There is currently one publication with column measurements that do not coincide with those listed above. Proceedings of the IEEE has a column measurement of 3.25 inches (82.5 millimeters/19.5 picas).

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E. Resolution

The proper resolution of your figures will depend on the type of figure it is as defined in the "Types of Figures" section. Author photographs, color, and grayscale figures should be at least 300dpi. Line art, including tables should be a minimum of 600dpi.

F. Vector Art

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The term color space refers to the entire sum of colors that can be represented within the said medium. For our purposes, the three main color spaces are Grayscale, RGB (red/green/blue) and CMYK (cyan/magenta/yellow/black). RGB is generally used with on-screen graphics, whereas CMYK is used for printing purposes.

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Multipliers can be especially confusing. Write "Magnetization (kA/m)" or "Magnetization (10^3 A/m)." Do not write "Magnetization (A/m) \times 1000" because the reader would not know whether the top axis label in Fig. 1 meant 16000 A/m or 0.016 A/m. Figure labels should be legible, approximately 8 to 10 point type.

2) Subfigure Labels in Multipart Figures and Tables: Multipart figures should be combined and labeled before final submission. Labels should appear centered below each subfigure in 8 point Times New Roman font in the format of (a) (b) (c).

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Figures (line artwork or photographs) should be named starting with the first 5 letters of the author's last name. The next characters in the filename should be the number that represents the sequential location of this image in your article. For example, in author "Anderson's" paper, the first three figures would be named ander1.tif, ander2.tif, and ander3.ps.

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Appendixes, if needed, appear before the acknowledgment.

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 - 2) J. K. Author, "Title of dissertation," Ph.D. dissertation, Abbrev. Dept., Abbrev. Univ., City of Univ., Abbrev. State, year.

See [25], [26].

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Month, year.

- 2) J. K. Author, "Title of paper," unpublished.
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- Example when using et al.: See [34].

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Dr. Author was a recipient of the International Association of Geomagnetism and Aeronomy Young Scientist Award for Excellence in 2008, and the IEEE Electromagnetic Compatibility Society Best Symposium Paper Award in 2011.



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Third C. Author, Jr. (M'87) received the B.S. degree in mechanical engineering from National Chung Cheng University, Chiayi, Taiwan, in 2004 and the M.S. degree in mechanical engineering from National Tsing Hua University, Hsinchu, Taiwan, in 2006. He is currently pursuing the Ph.D. degree in mechanical engineering at Texas A&M University, College Station, TX, USA.

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Mr. Author's awards and honors include the Frew Fellowship (Australian Academy of Science), the I. I. Rabi Prize (APS), the European Frequency and Time Forum Award, the Carl Zeiss Research Award, the William F. Meggers Award and the Adolph Lomb Medal (OSA).