

# Effects of error function selection and normalized fiber length range in numerical estimation of tendon slack length Hudson Burke, Xiao Hu Ph.D., Shawn Russell Ph.D.



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### INTRODUCTION

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  hd}$ In Hill-type muscle models, **tendon slack length (l\_s^t)** is a highly influential parameter.
- This value is **difficult to measure directly** because tendons often run parallel to muscle fibers.
- In simulations of **extreme motion**, force production is often **physiologically unreasonable.**
- Manal (2004) used an **optimization technique** to estimate muscle fiber lengths that would produce a consistent tendon slack length by deriving an **equation using architectural parameters and force-length curves** from Zajac (1989):

$$l_{s}^{t} = \frac{l^{mt} - l_{o}^{m} * \tilde{l}^{m} \cos \alpha}{\left[1 + \frac{\text{eval}[\tilde{F}_{\tilde{l}^{m}}^{m}] \cos \alpha + 0.2375}{37.5}\right]}$$

This research extends Manal's technique to analyze how different factors (like fiber length range and error functions) affect the estimation, aiming to create a more robust tuning methodology for new muscles and models.

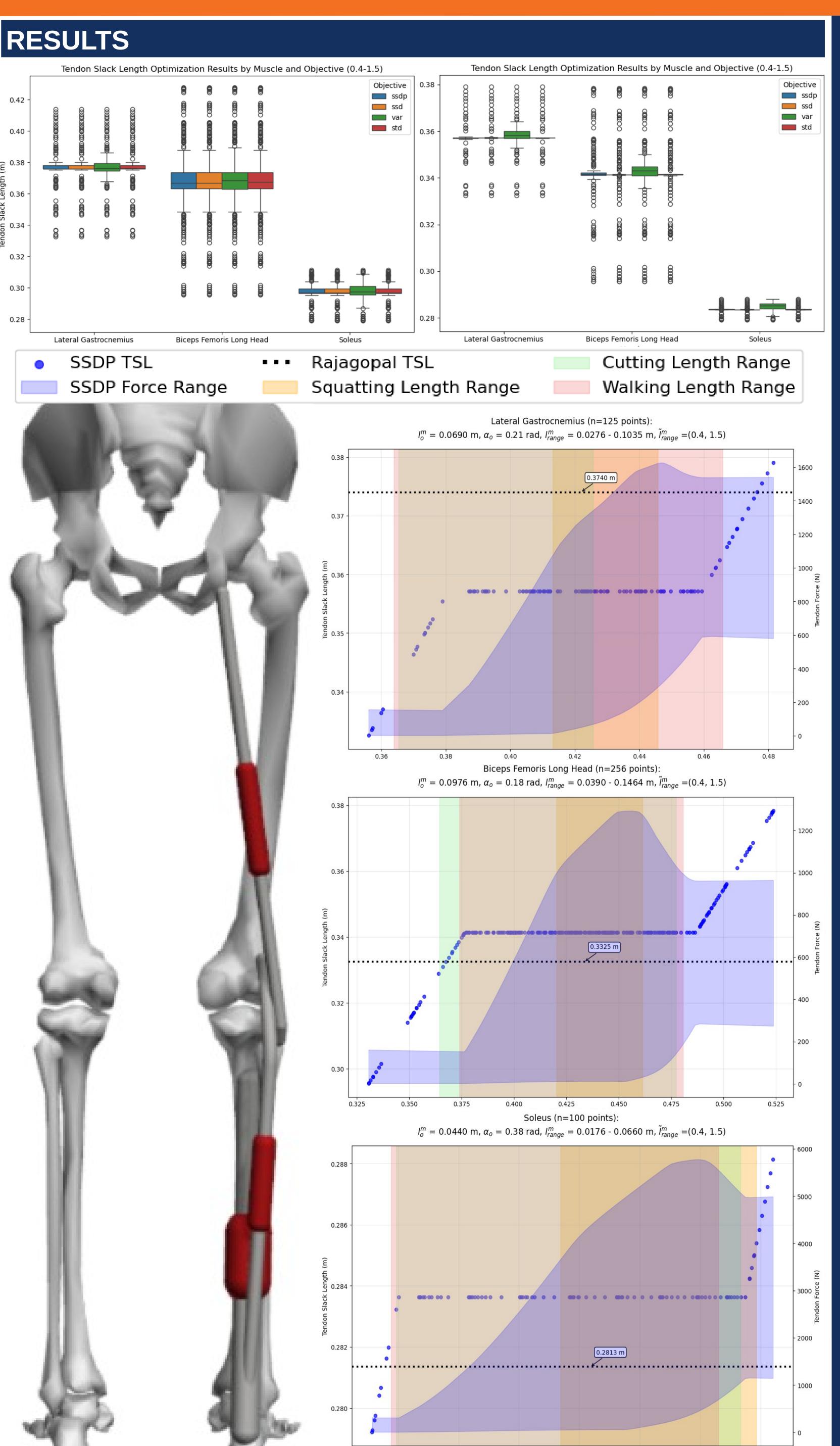
# AIMS

- 1) Identify different error functions for use in tendon slack length optimization
- 2) Analyze role of normalized fiber length range in tendon slack length estimation for different muscles

# METHODS

The refined approach uses:

- SLSQP (Sequential Least SQuares Programming) for optimization.
- Force-length curves from Millard et al.
- Musculotendon lengths sampled across the full range of motion of the RajagopalLaiUhlrich2023 model.
- Utilized four different error functions:
- •Sum of Squared Difference of Pairs (ssdp):  $\sum_i \sum_j ((i)l_s^t (j)l_s^t)^2$
- Sum of Squared Differences (ssd):  $\sum ({}_{(i)}l_s^t \bar{l}_s^t)^2$
- Standard Deviation (std):  $\sqrt{\frac{\sum (i)l_s^t \bar{l}_s^t)^2}{n}}$
- Variance (var):  $\frac{\sum (i)l_s^t \frac{1}{l_s^t})^2}{n}$
- Applied the methodology to the lateral gastrocnemius, biceps femoris long head, and soleus muscles.
- Ran the optimization on both the **full and the ascending-only portions** of the fiber force-length curve.



# DISCUSSION

- Changing the error functions produced little difference compared to each other, but the range of tendon slack length estimates changed substantially with normalized fiber length range.
- The tendon slack length plots **only show the estimates produced by SSDP**, used in Manal's original method.
- For each muscle, the tendon slack length estimated at each musculotendon length across a **normalized fiber** length range of 0.4 to 1.5 is plotted along with the corresponding force range.
- The **highlighted regions** show the range of musculotendon lengths in **different activities**, particularly an athletic cutting motion and squatting.
- In the middle of the musculotendon length range, a consistent value for tendon slack length emerges, but it deviates at the short and long ends of the range of motion
- The discrepancy comes as a result of the **constrained optimal fiber length range** as once the range reaches that limit, the tendon slack length is the only component that can compensate.
- This could introduce **activity dependent inaccuracies** when the musculotendon length is close to the ends of its range.
- For example, the tendon slack length estimate for the soleus may work for a squatting motion but not for an athletic cutting motion.

#### SIGNIFICANCE

- A comparison should be performed between the forces and lengths produced via this optimization method, and those using the values estimated in the standard Rajagopal model.
- Estimates for tendon slack length **must take into account the range of motion** used in the activity being analyzed and the corresponding musculotendon lengths to ensure consistency.
- Using time-series dynamic data in the future would allow the use of force-velocity curves in the optimization process which are currently neglected in this methodology and may become increasingly important with athletic motions.

#### References

Manal 2004, Journal of Applied Biomechanics
Zajac 1989, Critical Reviews in Biomedical Engineering
Rajagopal 2016, IEEE Transactions on Biomedical Engineering
Uhlrich 2022, Scientific Reports
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Silder 2007, Journal of Biomechanics

