

# AFIRT: A Dimensionless Potency Metric for Characterizing the Activity of Monoclonal Antibodies in Target Tissue

Abstract Word Count: XYZ

Body Word Count (including figure captions): XYZ

Number of Figures: XYZ

Number of Tables: XYZ

Keywords: monoclonal antibody | target mediated drug disposition | pharmacokinetics and pharmacodynamics | pharmacometrics

Andrew M. Stein<sup>1</sup>, Sameed Ahmed<sup>2</sup>, Miandra Ellis<sup>3</sup>, Ngartelbaye Guerngar<sup>4</sup>,  
Hongshan Li<sup>5</sup>, Luca Pallucchini<sup>6</sup>

## Contents

<b>1 Rough outline</b>	<b>3</b>
<b>2 Introduction</b>	<b>3</b>
<b>3 Theory</b>	<b>4</b>
3.1 Model Description . . . . .	4
3.2 AFIRT derivation . . . . .	6
3.2.1 Membrane-bound Target . . . . .	7
3.2.2 Soluble target at Initial State and Steady State . . . . .	7
<b>4 Methods and Results</b>	<b>9</b>
<b>5 Discussion</b>	<b>9</b>
<b>6 Conclusion</b>	<b>9</b>
<b>7 Appendix</b>	<b>9</b>
7.1 Predicting drug concentration in tissue ( $D_{\text{tot,avg3}}$ ) . . . . .	9
7.2 Predicting Target accumulation in Target Tissue ( $M_{\text{acc3}}$ ) . . . . .	10
7.3 Similarity Transform . . . . .	11

<sup>1</sup>Novartis Institute for BioMedical Research, 45 Sidney St, Cambridge MA, 02140 USA,  
andrew.stein@novartis.com

<sup>2</sup>Departments of Mathematics, University of South Carolina, ahmed3@math.sc.edu

<sup>3</sup>School of Mathematical and Statistical Sciences, Arizona State University, melis5@asu.edu

<sup>4</sup>Department of Mathematics and Statistics, Auburn University, nzg0017@auburn.edu

<sup>5</sup>Department of Mathematics, Purdue University, li108@purdue.edu

<sup>6</sup>Department of Mathematics, Temple University, luca.pallucchini@temple.edu

**8 Figures and Tables****15**

Figure are in a separate file at the end of this document. They'll images themselves will need to be removed for CPT:PSP (06-Figures.tex).

**Abstract**

XYZ

# 1 Rough outline

In this paper we will:

- derive AFIRT
  - new result = AFIRT formula
  - new result = Kssd
- use sensitivity analysis to confirm AFIRT formula and show when it fails
  - large receptor concentration (herceptin = trastuzumab)
- specific practical results from AFIRT and sensitivity analysis
  - demonstrate the importance of understanding tissue-accumulation (bevacizumab)
  - explore how fast shed rate needs to be to limit inhibition
- discussion
  - practical value - don't need every microconstant, just a few lumped parameter estimates
  - don't need a complex physiological model, the simple formula can work well
  - essentially, Kssd should have been used for atezo instead of Kd

# 2 Introduction

In the development of biologics, understanding target engagement at the site of action plays a critical role in dose regimen selection [1]. As measurements at the site of action are often impossible to obtain, model based predictions of target engagement at the site of action are often used to help justify the dose regimen selection. For the PD-1 inhibitor pembrolizumab, a physiologically based model for antibody distribution and target engagement was developed to predict the dose needed to achieve target engagement and tumor suppression [2]. For the PD-L1 inhibitor atezolizumab, a much simpler approach was taken to help justify the dose regimen, where a particular tumor biodistribution coefficient ( $B$ ) and in vivo binding affinity ( $K_d$ ) was assumed, the steady state trough concentration ( $C_{\min}$ ) was estimated from clinical observations, and then the receptor occupancy ( $RO$ ) formula in Equation 1 was used to identify the dosing regimen that would provide the drug concentration needed to achieve 95% target occupancy.

$$RO = B \cdot C_{\min} / (B \cdot C_{\min} + K_d) \quad (1)$$

The advantage of using the complex, mechanistic model as done for pembrolizumab is that ideally, it captures all essential underlying physiology processes in making the dose regimen prediction. The disadvantage of this approach

is that physiological models can be complex, making them difficult time consuming to develop, difficult to accurately estimate all model parameters, and difficult to explain to collaborators. The advantage using the simple  $RO$  formula as done for atezolizumab is that it is fast, easy to implement, and easy to explain to collaborators. The disadvantage is that it is not immediately obvious that Equation 1 is the appropriate equation to use to describe the clinical scenario as this equation was derived for the in vitro setting [3] where there was no drug distribution, target distribution, receptor synthesis, or receptor shedding.

In this paper, a mathematical analysis of the target mediated drug distribution system is performed with the goal of deriving a simple expression for target engagement in the clinical scenario. This work provides a simple expression for target engagement in the tissue of interest, extending previous work characterizing the Average Free target to Initial target Ratio (AFIR) at steady state in circulation [4].

PROVIDE AN OUTLINE OF THE PAPER HERE

### 3 Theory

In this section, an expression for the average free target to initial target ratio in tissue (AFIRT) is derived for the model in Figure 1.

#### 3.1 Model Description

The model in Figure 1 is based on the standard TMDD model [5, 4], where a drug ( $D$ ) binds its target, but it has been extended to include the following processes:

- Shedding of the membrane bound target ( $M$ ) into soluble target ( $S$ ).
- The drug can bind both the soluble target and the membrane-bound target to form complexes  $DS$  and  $DM$  respectively.
- Both the soluble and membrane-bound target are present in both the central compartment (1) and a tissue compartment (3).
- Soluble target is able to distribute between the central and tissue compartment (e.g. passive diffusion of target molecules)
- Membrane-bound target is able to distribute between central and tissue compartment (e.g. active trafficking of immune cells expressing the membrane-bound target).

As with the standard TMDD model, the peripheral compartment (2) contains the drug only; it is included so that the two-compartment pharmacokinetics of the drug can be described. This model is more complex than most physiological models in the literature. Often, trafficking of the membrane-bound target is ignored and often, either the soluble or membrane-bound target is modeled but

not both. In this paper, an analysis of this complete model is performed. The simpler scenarios can easily be represented using this model and setting the appropriate parameters to zero.

The ordinary differential equations for describing this system are summarized below.

$$\begin{aligned} \frac{dD_1}{dt} = & \frac{1}{V_C} \text{Dose}_{iv}(t) - k_{12D} D_1 + \frac{V_{D_2}}{V_{D_1}} k_{21D} D_2 - k_{13D} D_1 + \frac{V_{D_3}}{V_{D_1}} k_{31D} D_3 \\ & - k_{eD1} D_1 - k_{on1} D_1 \cdot S_1 + k_{off1}(DS_1) - k_{on1} D_1 \cdot M_1 + k_{off1}(DM_1) \end{aligned} \quad (2)$$

$$\frac{dD_2}{dt} = k_{12D} \frac{V_{D_1}}{V_{D_2}} D_1 - k_{21D} D_2 \quad (3)$$

$$\begin{aligned} \frac{dD_3}{dt} = & \frac{V_{D_1}}{V_{D_3}} k_{13D} D_1 - k_{31D} D_3 - k_{eD3} D_3 - k_{on3} D_3 \cdot M_3 + k_{off3}(DM_3) \\ & - k_{on3} D_3 \cdot S_3 + k_{off3}(DS_3) \end{aligned} \quad (4)$$

$$\begin{aligned} \frac{dM_1}{dt} = & k_{synM1} - k_{shedM1} M_1 - k_{13M} M_1 + \frac{V_{M_3}}{V_{M_1}} k_{31M} M_3 - k_{eM1} M_1 \\ & - k_{on1} D_1 \cdot M_1 + k_{off1}(DM_1) \end{aligned} \quad (5)$$

$$\begin{aligned} \frac{dM_3}{dt} = & k_{syn3} - k_{shedM3} M_3 + \frac{V_{M_1}}{V_{M_3}} k_{13M} M_1 - k_{31M} M_3 - k_{eM3} M_3 - \\ & k_{on3} D_3 \cdot M_3 + k_{off3}(DM_3) \end{aligned} \quad (6)$$

$$\begin{aligned} \frac{dS_1}{dt} = & k_{synS1} + k_{shedM1} M_1 - k_{13S} S_1 + \frac{V_{S_3}}{V_{S_1}} k_{31S} S_3 - k_{eS1} S_1 - k_{on1} D_1 \cdot S_1 \\ & + k_{off1}(DS_1) \end{aligned} \quad (7)$$

$$\begin{aligned} \frac{dS_3}{dt} = & k_{synS3} + k_{shedM3} M_3 - k_{31S} S_3 + \frac{V_{S_1}}{V_{S_3}} k_{13S} S_1 - k_{eS3} S_3 - k_{on3} D_3 \cdot S_3 \\ & + k_{off3}(DS_3) \end{aligned} \quad (8)$$

$$\begin{aligned} \frac{d(DM_1)}{dt} = & -k_{shedDM1} DM_1 - k_{13DM}(DM_1) + \frac{V_{DM_3}}{V_{DM_1}} k_{31DM}(DM_3) - k_{eDM1} DM_1 \\ & + k_{on1} D_1 \cdot M_1 - k_{off1}(DM_1) \end{aligned} \quad (9)$$

$$\begin{aligned} \frac{d(DM_3)}{dt} = & -k_{shedDM3} DM_3 - k_{31DM}(DM_3) + \frac{V_{DM_1}}{V_{DM_3}} k_{13DM}(DM_1) - k_{eDM3} DM_3 \\ & + k_{on3} D_3 \cdot M_3 - k_{off3}(DM_3) \end{aligned} \quad (10)$$

$$\begin{aligned} \frac{d(DS_1)}{dt} = & -k_{shedDM3} DS_1 - k_{13DS} DS_1 + \frac{V_{DS_3}}{V_{DS_1}} k_{31DS} DS_3 - k_{eDS1}(DS_1) \\ & + k_{on1} D_1 \cdot S_1 - k_{off1}(DS_1) \end{aligned} \quad (11)$$

$$\begin{aligned} \frac{d(DS_3)}{dt} = & -k_{shedDM3} DS_3 - k_{31DS} DS_3 + \frac{V_{DS_1}}{V_{DS_3}} k_{13DS} DS_1 - k_{eDS3}(DS_3) \\ & + k_{on3} D_1 \cdot S_3 - k_{off1}(DS_3) \end{aligned} \quad (12)$$

For the first time we are calculating the AFIRT using an alternative ap-

proximations to the quasi-equilibrium (QE), the quasi-steady state (QSS) and the quasi-steady state xxxxxxxx (QSSD). The quasi-steady state approximation assumed that  $-k_{\text{shed}DM_3}DM_3 - k_{eDM3}DM_3 + k_{\text{on}3}D_3 \cdot M_3 - k_{\text{off}3}(DM_3) = 0$ , similarly as before for  $k_d$  we define  $k_{ss} = \frac{k_{\text{shed}DM_3} + k_{eDM3} + k_{\text{off}3}}{k_{\text{on}3}}$ .

#### DESCRIBE THE INITIAL CONDITIONS OF THE MODEL

### 3.2 AFIRT derivation

I PROPOSE THAT THIS SECTION START WITH A HIGH LEVEL OVERVIEW OF THE STEPS TO CALCULATE AFIRT. THEN, THESE STEPS CAN EITHER BE REPRODUCED IN THE MAIN BODY OR IN THE APPENDIX.

#### KEY STEPS

- Focus on steady state for a constant infusion.
- Assume the drug concentration is very large
- Calculate drug concentration in tissue at steady state  $D_{\text{tot},\text{avg}3,\text{ss}} = C_{\text{avg}3,\text{ss}} = B \cdot C_{\text{avg}1,\text{ss}} = D_{\text{tot},\text{avg}1,\text{ss}}$ .
  - For large drug concentration, target kinetics can be ignored.
  - Use the similarity transform to remove  $k_{eD3}$ .
  - This gives us a simple expression for  $C_{\text{avg}1} = D_{\text{tot},\text{avg}1}$  as a function of  $CL$ .
  - This also gives us an expression for  $B$  such that  $C_{\text{avg}3} = D_{\text{tot},\text{avg}3} = B \cdot C_{\text{avg}1}$ .
- Calculate target concentration in tissue at steady state.
  - For large drug concentration, drug kinetics can be ignored.
  - Do the small matrix algebra inversion to calculate  $M_{30}$  and  $M_{3\text{tot},\text{ss}}$ .
  - Calculate accumulation factor
- Calculate the free fraction by assuming various processes are slow/fast.
  - $K_d$
  - $K_{ss}$
  - $K_{\text{ssd}}$
- Putting this all together gives  $AFIRT_M$ .
- A similar process can be followed for  $AFIRT_S$ .

### 3.2.1 Membrane-bound Target

The quasi-steady state approximation assumed that  $-k_{\text{shed}DM_3}DM_3 - k_{31DM}(DM_3) - k_{eDM3}DM_3 + k_{\text{on}3}D_3 \cdot M_3 - k_{\text{off}3}(DM_3) = 0$ , we define  $k_{ssd} = \frac{k_{\text{shed}DM_3} + k_{31DM} + k_{eDM3} + k_{\text{off}3}}{k_{\text{on}3}}$ . These approximations are obtained from equation (16) at steady state, i.e.  $\frac{d(DM_3)}{dt} = 0$ , and assuming the terms  $\frac{V_{DM_1}}{V_{DM_3}}k_{13DM}(DM_1)$  and  $k_{31DM}(DM_3)$  are negligible for the QSS. We assume that only  $\frac{V_{DM_1}}{V_{DM_3}}k_{13DM}(DM_1)$  is negligible for the QSSD.

We obtain the following approximations

$$\begin{aligned}\text{AFIRT} &\approx k_{ssd} \frac{M_{3\text{tot,ss}}}{M_{3,0}} \frac{\text{CL} \times \tau}{\text{B} \times \text{Dose}}, \\ \text{AFIRT} &\approx k_{ss} \frac{M_{3\text{tot,ss}}}{M_{3,0}} \frac{\text{CL} \times \tau}{\text{B} \times \text{Dose}}, \\ \text{AFIRT} &\approx k_d \frac{M_{3\text{tot,ss}}}{M_{3,0}} \frac{\text{CL} \times \tau}{\text{B} \times \text{Dose}},\end{aligned}$$

where

$$\begin{aligned}M_{3\text{tot,ss}} &= \frac{k_{13DM}(V_C/V_T)k_{\text{syn}M1} + (k_{eDM1} + k_{\text{shed}DM1} + k_{13DM})k_{\text{syn}M3}}{(k_{eDM1} + k_{\text{shed}DM1} + k_{13DM})(k_{eDM3} + k_{\text{shed}DM3} + k_{31DM}) - k_{31DM}k_{13DM}}, \\ M_{3,0} &= \frac{k_{13M}(V_C/V_T)k_{\text{syn}M1} + (k_{eM1} + k_{\text{shed}M1} + k_{13M})k_{\text{syn}M3}}{(k_{eM1} + k_{\text{shed}M1} + k_{13M})(k_{eM3} + k_{\text{shed}M3} + k_{31M}) - k_{31M}k_{13M}}, \\ \text{B} &= \frac{k_{13D}(V_C/V_T)}{k_{eD3} + k_{31D}}.\end{aligned}$$

We can notice from the picture below that the approximation obtained using the (QSS) hypothesis gives better results than the one using (QE).

### 3.2.2 Soluble target at Initial State and Steady State

With the same notations as in the sections above.

**At initial state**, we have

$$\begin{aligned}\frac{dS_1}{dt} &= 0 \\ \frac{dS_3}{dt} &= 0 \\ M_1 &= M_{10} \\ M_3 &= M_{30} \\ D_1 &= 0 \\ D_3 &= 0 \\ DS_1 &= 0 \\ DS_3 &= 0\end{aligned}$$

So ODE 13 and 14 give us the following linear system

$$\begin{bmatrix} -(k_{13S} + k_{eS1}) & \frac{V_T}{V_C} k_{31S} \\ \frac{V_C}{V_T} k_{13S} & -(k_{31S} + k_{eS3}) \end{bmatrix} \cdot \begin{bmatrix} S_1 \\ S_3 \end{bmatrix}_0 = \begin{bmatrix} -k_{synS1} - k_{shedM1} M_{10} \\ -k_{synS3} - k_{shedM3} M_{30} \end{bmatrix}.$$

So the initial soluble target concentration in the central and tumor compartment is

$$S_{10} = \frac{(k_{31S} + k_{eS3}) \cdot (k_{synS1} + k_{shedM1} M_{10}) + \frac{V_T}{V_C} k_{31S} (k_{synS3} + k_{shedM3} M_{30})}{(k_{13S} + k_{eS1})(k_{31S} + k_{eS3}) - k_{13S} k_{31S}} \quad (13)$$

$$S_{30} = \frac{\frac{V_C}{V_T} \cdot k_{13S} \cdot (k_{synS1} + k_{shedM1} M_{10}) + (k_{13S} + k_{eS1})(k_{synS3} + k_{shedM3} M_{30})}{(k_{13S} + k_{eS1})(k_{31S} + k_{eS3}) - k_{13S} k_{31S}}. \quad (14)$$

**At steady state**, we assume that all soluble target are in the form of bounded complex. By the symmetry of our model, we have

$$S_{1tot,ss} = \frac{(k_{31DS} + k_{eDS3}) \cdot (k_{synS1} + k_{shedDM1} M_{1tot,ss}) + \frac{V_T}{V_C} k_{31DS} (k_{synS3} + k_{shedDM3} M_{3tot,ss})}{(k_{13DS} + k_{eDS1})(k_{31DS} + k_{eDS3}) - k_{13DS} k_{31DS}}$$

$$S_{3tot,ss} = \frac{\frac{V_C}{V_T} k_{13DS} \cdot (k_{synS1} + k_{shedDM1} M_{1tot,ss}) + (k_{13DS} + k_{eDS1})(k_{synS3} + k_{shedDM3} M_{3tot,ss})}{(k_{13DS} + k_{eDS1})(k_{31DS} + k_{eDS3}) - k_{13DS} k_{31DS}}$$

Formulas for computing membrane target at initial and steady state can be found in *Model F Appendix*, for convenience, we include them below

$$M_{10} = \frac{(k_{shedM3} + k_{31M} + k_{eM3}) k_{synM1} + \frac{V_T}{V_C} k_{31M} k_{synM3}}{(k_{shedM1} + k_{13M} + k_{eM1})(k_{shedM3} + k_{31M} + k_{eM3}) - k_{13M} k_{31M}}$$

$$M_{30} = \frac{\frac{V_C}{V_T} k_{13M} k_{synM1} + (k_{shedM1} + k_{13M} + k_{eM1}) k_{synM1}}{(k_{shedM1} + k_{13M} + k_{eM1})(k_{shedM3} + k_{31M} + k_{eM3}) - k_{13M} k_{31M}}$$

$$M_{1tot,ss} = \frac{(k_{shedDM3} + k_{31DM} + k_{eDM3}) k_{synM1} + \frac{V_T}{V_C} k_{31DM} k_{synM3}}{(k_{shedDM1} + k_{13DM} + k_{eDM1})(k_{shedDM3} + k_{31DM} + k_{eDM3}) - k_{13DM} k_{31DM}}$$

$$M_{3tot,ss} = \frac{\frac{V_C}{V_T} k_{13DM} k_{synM1} + (k_{shedDM1} + k_{13DM} + k_{eDM1}) k_{synM1}}{(k_{shedDM1} + k_{13DM} + k_{eDM1})(k_{shedDM3} + k_{31DM} + k_{eDM3}) - k_{13DM} k_{31DM}}$$

The formulas to compute various AFIRTS for soluble targets in the tumor compartment are

$$\text{AFIRTS.Kssd} = \text{Kssd.S} \times \frac{\text{Tacc.tum.S}}{\text{B} \times C_{avg1}} \quad (15)$$

$$\text{AFIRTS.Kss} = \text{Kss.S} \times \frac{\text{Tacc.tum.S}}{\text{B} \times C_{avg1}} \quad (16)$$

$$\text{AFIRTS.Kd} = \text{Kd.S} \times \frac{\text{Tacc.tum.S}}{\text{B} \times C_{avg1}} \quad (17)$$

$$(18)$$

Where  $K_{ssd,S}$ ,  $K_{ss,S}$  and  $K_{d,S}$

$$K_{ssd,S} = \frac{k_{shedDM3} + k_{31DS} + k_{eDS} + k_{off3}}{k_{on3}} \quad (19)$$

$$K_{ss,S} = \frac{k_{shedDM3} + k_{eDS} + k_{off3}}{k_{on3}} \quad (20)$$

$$K_{d,S} = \frac{k_{off3}}{k_{on3}} \quad (21)$$

(22)

Finally,

$$T_{acc,tum,S} = S_3 \text{tot,ss}/S_{30} \quad (23)$$

To compute AFIRT for soluable target from simulation, do

1. compute  $S_{free,pct} := \frac{S_3}{S_{30}}$
2. take the average of  $S_{free,pct}$  in the steady state
3. return the result from step 2

## 4 Methods and Results

## 5 Discussion

## 6 Conclusion

## 7 Appendix

### 7.1 Predicting drug concentration in tissue ( $D_{\text{tot,avg3}}$ )

Ignoring target, then at steady state

$$\begin{aligned} - \begin{pmatrix} k_{inf} \\ 0 \\ 0 \end{pmatrix} &= \frac{d}{dt} \begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix} = \begin{pmatrix} -(k_{eD1} + k_{12D} + k_{13D}) & (V_P/V_C)k_{21D} & (V_T/V_C)k_{31D} \\ (V_C/V_P)k_{12D} & -k_{21D} & 0 \\ (V_C/V_T)k_{13D} & 0 & -(k_{eD3} + k_{31D}) \end{pmatrix} \cdot \begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix} \\ &= A \cdot \begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix} \end{aligned}$$

$B$  is given by the ratio of  $D_{3,ss}/D_{1,ss}$  at steady state.

$$\begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix}_{ss} = A^{-1} \cdot \begin{pmatrix} -k_{inf} \\ 0 \\ 0 \end{pmatrix}$$

$$\begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix}_{ss} = \frac{-k_{\text{inf}}}{\det A} \begin{pmatrix} a_{22}a_{33} - a_{23}a_{32} \\ a_{23}a_{31} - a_{21}a_{33} \\ a_{21}a_{32} - a_{22}a_{31} \end{pmatrix} = \begin{pmatrix} k_{21D}(k_{eD3} + k_{31D}) \\ k_{21D}(V_P/V_C)(k_{eD3} + k_{31D}) \\ k_{21D}(V_C/V_T)k_{13D} \end{pmatrix}$$

And finally, the biodistribution coefficient for tissue 3 is given by:

$$B = \left( \frac{D_3}{D_1} \right)_{ss} = \frac{k_{21D}(V_C/V_T)k_{13D}}{k_{21D}(k_{eD3} + k_{31D})} = \frac{V_C}{V_T} \cdot \frac{k_{13D}}{(k_{eD3} + k_{31D})}$$

Thus in the limits prescribed above, where target expression does not effect drug distribution, we have:

$$D_{\text{tot,avg3}} = B \cdot D_{\text{tot,avg1}}$$

## 7.2 Predicting Target accumulation in Target Tissue ( $M_{\text{acc3}}$ )

Before the drug is given, the initial steady state target levels can be computed by solving the system below:

$$\begin{pmatrix} 0 \\ 0 \end{pmatrix} = \frac{d}{dt} \begin{pmatrix} M_1 \\ M_3 \end{pmatrix} = \begin{pmatrix} -(k_{eM1} + k_{13M} + k_{\text{shed}M_1}) & (V_T/V_C)k_{31M} \\ (V_C/V_T)k_{13T} & -(k_{eM3} + k_{31M} + k_{\text{shed}M_3}) \end{pmatrix} \begin{pmatrix} M_1 \\ M_3 \end{pmatrix}_0 + \begin{pmatrix} k_{\text{syn}1} \\ k_{\text{syn}3} \end{pmatrix}$$

$$\begin{pmatrix} k_{\text{syn}1} \\ k_{\text{syn}3} \end{pmatrix} = \begin{pmatrix} (k_{eM1} + k_{13M} + k_{\text{shed}M_1}) & -(V_T/V_C)k_{31M} \\ -(V_C/V_T)k_{13M} & (k_{eM3} + k_{31M} + k_{\text{shed}M_3}) \end{pmatrix} \begin{pmatrix} M_1 \\ M_3 \end{pmatrix}_0$$

Then, using the formula for inverting a 2d matrix gives

$$\begin{pmatrix} M_1 \\ M_3 \end{pmatrix}_0 = \frac{1}{((k_{eM3} + k_{31M} + k_{\text{shed}M_3})(k_{eM1} + k_{13M} + k_{\text{shed}M_1}) - k_{13T}k_{31T})} \times$$

$$\begin{pmatrix} (k_{eM3} + k_{31M} + k_{\text{shed}M_3}) & (V_T/V_C)k_{31M} \\ (V_C/V_T)k_{13M} & (k_{eM1} + k_{13M} + k_{\text{shed}M_1}) \end{pmatrix} \begin{pmatrix} k_{\text{syn}1} \\ k_{\text{syn}3} \end{pmatrix}$$

The key parameter of interest is the target expression in the tissue of interest:

$$M_{3,0} = \frac{k_{13M}(V_C/V_T)k_{\text{syn}M1} + (k_{eM1} + k_{\text{shed}M_1} + k_{13M})k_{\text{syn}3}}{(k_{eM1} + k_{\text{shed}M_1} + k_{13M})(k_{eM3} + k_{\text{shed}M_3} + k_{31M}) - k_{31M}k_{13M}}$$

If we assume that the drug is in vast excess to the amount of target and that almost all the target is present as bound to drug, then the total target kinetics can be described by the same set of equations above, but replacing all  $M$  terms with  $DM$  terms, giving

$$M_{3\text{tot,ss}} = \frac{k_{13DM}(V_C/V_T)k_{\text{syn}M1} + (k_{eDM1} + k_{\text{shed}DM_1} + k_{13DM})k_{\text{syn}3}}{(k_{eDM1} + k_{\text{shed}DM_1} + k_{13DM})(k_{eDM3} + k_{\text{shed}DM_3} + k_{31DM}) - k_{31DM}k_{13DM}}$$

Then, to compute  $M_{\text{acc3}}$  just take the ratio of  $M_{\text{tot3}}/M_{03}$

$$M_{\text{acc3}} = \frac{M_{\text{tot3}}}{M_{03}} = \frac{k_{13DM}(V_C/V_T)k_{\text{syn}M1} + (k_{eDM1} + k_{\text{shed}DM_1} + k_{13DM})k_{\text{syn}3}}{(k_{eDM1} + k_{\text{shed}DM_1} + k_{13DM})(k_{eDM3} + k_{\text{shed}DM_3} + k_{31DM}) - k_{31DM}k_{13DM}} \times$$

$$\frac{(k_{eM1} + k_{\text{shed}M_1} + k_{13M})(k_{eM3} + k_{\text{shed}M_3} + k_{31M}) - k_{31M}k_{13M}}{k_{13M}(V_C/V_T)k_{\text{syn}M1} + (k_{eM1} + k_{\text{shed}M_1} + k_{13M})k_{\text{syn}3}}$$

### 7.3 Similarity Transform

We consider the model in Figure 1. A drug ( $D$ ) binds to its target ( $M$ ) to form a complex ( $DM$ ). It has three compartments, central, tissue, and peripheral.

The drug and target dynamics are modeled with the following system of ordinary differential equations

$$\begin{aligned} \frac{dD_1}{dt} &= \frac{1}{V_1} \text{Dose}_{iv}(t) - k_{12D} D_1 + \frac{V_3}{V_1} k_{21D} D_2 - k_{13D} D_1 \\ &\quad + \frac{V_2}{V_1} k_{31D} D_3 - k_{on1} D_1 \cdot M_1 + k_{off1}(DM_1) - k_{eD1} D_1 \end{aligned} \quad (24)$$

$$\frac{dD_2}{dt} = k_{12D} \frac{V_1}{V_3} D_1 - k_{21D} D_2 \quad (25)$$

$$\frac{dD_3}{dt} = \frac{V_1}{V_2} k_{13D} D_1 - k_{31D} D_3 - k_{on3} D_3 \cdot M_3 + k_{off3}(DM_3) - k_{eD3} D_3 \quad (26)$$

$$\begin{aligned} \frac{dM_1}{dt} &= k_{syn1} - k_{13M} M_1 + \frac{V_2}{V_1} k_{31M} M_3 - k_{on1} D_1 \cdot M_1 + k_{off1}(DM_1) \\ &\quad - k_{eM1} M_1 \end{aligned} \quad (27)$$

$$\begin{aligned} \frac{dM_3}{dt} &= k_{syn3} + \frac{V_1}{V_2} k_{13M} M_1 - k_{31M} M_3 - k_{on3} D_3 \cdot M_3 + k_{off3}(DM_3) \\ &\quad - k_{eM3} M_3 \end{aligned} \quad (28)$$

$$\begin{aligned} \frac{d(DM_1)}{dt} &= -k_{13DM}(DM_1) + \frac{V_2}{V_1} k_{31DM}(DM_3) + k_{on1} D_1 \cdot M_1 - k_{off1}(DM_1) \\ &\quad - k_{eDM1}(DM_1) \end{aligned} \quad (29)$$

$$\begin{aligned} \frac{d(DM_3)}{dt} &= \frac{V_1}{V_2} k_{13DM}(DM_1) - k_{31DM}(DM_3) + k_{on3} D_3 \cdot M_3 - k_{off3}(DM_3) \\ &\quad - k_{eDM3}(DM_3) \end{aligned} \quad (30)$$

(31)

We will calculate  $D_{tot,avg3}$ , which is the average drug concentration at steady state in the tissue. We have  $D_{tot,avg3} = B \cdot D_{tot,avg1}$ , where  $D_{tot,avg1}$  is the average drug concentration at steady state in the central, and  $B$  is the antibody biodistribution coefficient. Assume that drug elimination only occurs in the central compartment, i.e.,  $k_{eD3} = 0$ . Then for drugs dosed with linear PK at regular intervals and concentration much larger than target concentration, we have  $D_{tot,avg1} = \text{Dose}/(CL \cdot \tau)$ , where  $CL = k_{eD1} \cdot V_1$  is the drug clearance [CITE REFERENCE 25 FROM AFIR ARTICLE].

For the model with drug elimination in both the central and tissue compartments, we will derive an alternative model with  $k_{eD3} = 0$  that is indistinguishable from the existing model by using the similarity transform technique [CITE GODFREY 1989]. We consider drug concentration large enough that target binding does not affect drug distribution. Then the model equations for

the drug can be written as

$$\frac{d\mathbf{D}}{dt} = A \cdot \mathbf{D}(t) + B \cdot Dose_{iv}(t), \quad (32)$$

with measurement

$$\mathbf{m}(t) = C \cdot \mathbf{D}(t), \quad (33)$$

where

$$\mathbf{D} = \begin{pmatrix} D_1 \\ D_2 \\ D_3 \end{pmatrix}, \quad (34)$$

$$A = \begin{pmatrix} -(k_{13D} + k_{12D} + k_{eD1}) & \frac{V_3}{V_1} k_{21D} & \frac{V_2}{V_1} k_{31D} \\ \frac{V_1}{V_2} k_{12D} & -k_{21D} & 0 \\ \frac{V_1}{V_2} k_{13D} & 0 & -(k_{31D} + k_{eD3}) \end{pmatrix}, \quad (35)$$

$$B = \begin{pmatrix} \frac{1}{V_1} \\ 0 \\ 0 \end{pmatrix}, \quad (36)$$

$$C = \begin{pmatrix} 1 & 0 & 0 \\ 0 & 0 & 1 \end{pmatrix}. \quad (37)$$

We transform this model into an indistinguishable model with coefficient matrices  $A'$ ,  $B'$ , and  $C'$  such that  $k'_{eD3} = 0$ . This is accomplished with the similarity transform

$$A' := TAT^{-1} \quad B' := TB \quad C' := CT^{-1}, \quad (38)$$

for some transformation matrix

$$T = \begin{pmatrix} t_{11} & t_{12} & t_{13} \\ t_{21} & t_{22} & t_{23} \\ t_{31} & t_{32} & t_{33} \end{pmatrix} \quad T^{-1} = \begin{pmatrix} \hat{t}_{11} & \hat{t}_{12} & \hat{t}_{13} \\ \hat{t}_{21} & \hat{t}_{22} & \hat{t}_{23} \\ \hat{t}_{31} & \hat{t}_{32} & \hat{t}_{33} \end{pmatrix}. \quad (39)$$

Alternatively, one can get this similarity transform with the change of variables  $\mathbf{D} = T^{-1}\mathbf{D}'$ . Then from (32) and (33) we have

$$\frac{d(T^{-1}\mathbf{D}')}{dt} = A \cdot (T^{-1}\mathbf{D}')(t) + B \cdot Dose_{iv}(t), \quad \mathbf{m}(t) = C \cdot (T^{-1}\mathbf{D}')(t). \quad (40)$$

Multiplying the first equation in (40) on the left by  $T$  yields

$$\frac{d\mathbf{D}'}{dt} = TAT^{-1} \cdot \mathbf{D}'(t) + TB \cdot Dose_{iv}(t). \quad (41)$$

Then we have the new model equation and measurement

$$\frac{d\mathbf{D}'}{dt} = A' \cdot \mathbf{D}'(t) + B' \cdot Dose_{iv}(t), \quad \mathbf{m}(t) = C' \cdot \mathbf{D}'(t), \quad (42)$$

where  $A'$ ,  $B'$ , and  $C'$  are given by (38).

Regardless of model formulation, the same dose is given to  $D_1$ , that is,

$$B' = B. \quad (43)$$

From this and (38) we get  $t_{11} = 1$ ,  $t_{21} = 0$ , and  $t_{31} = 0$ . Regardless of model formulation, we measure  $D_1$  and  $D_3$ , that is,

$$C' = C. \quad (44)$$

From this and (38) we get  $\hat{t}_{11} = 1$ ,  $\hat{t}_{12} = 0$ ,  $\hat{t}_{13} = 0$ ,  $\hat{t}_{31} = 0$ ,  $\hat{t}_{32} = 0$ , and  $\hat{t}_{33} = 1$ . For a  $3 \times 3$  matrix, the inverse is given by

$$T^{-1} = \frac{1}{\det T} \begin{pmatrix} t_{22}t_{33} - t_{23}t_{32} & t_{13}t_{32} - t_{12}t_{33} & t_{12}t_{23} - t_{13}t_{22} \\ t_{23}t_{31} - t_{21}t_{33} & t_{11}t_{33} - t_{13}t_{31} & t_{13}t_{21} - t_{11}t_{23} \\ t_{21}t_{32} - t_{22}t_{31} & t_{12}t_{31} - t_{11}t_{32} & t_{11}t_{22} - t_{12}t_{21} \end{pmatrix}, \quad (45)$$

with the determinant given by

$$\det T = t_{11}(t_{22}t_{33} - t_{23}t_{32}) - t_{12}(t_{21}t_{33} - t_{23}t_{31}) + t_{13}(t_{21}t_{32} - t_{22}t_{31}). \quad (46)$$

Putting the above findings into  $T^{-1}$  yields  $t_{12} = 0$ ,  $t_{13} = 0$ ,  $t_{32} = 0$ , and  $t_{33} = 1$ . From  $TT^{-1} = I$ , we get  $t_{22} = 1$ . Then we have

$$T = \begin{pmatrix} 1 & 0 & 0 \\ 0 & 1 & t_{23} \\ 0 & 0 & 1 \end{pmatrix} \quad T^{-1} = \begin{pmatrix} 1 & 0 & 0 \\ 0 & 1 & -t_{23} \\ 0 & 0 & 1 \end{pmatrix}. \quad (47)$$

Putting this into (38) yields

$$A' = \begin{pmatrix} -(k_{13D} + k_{12D} + k_{eD1}) & \frac{V_3}{V_1}k_{21D} & -\frac{V_3}{V_1}k_{21D}t_{23} + \frac{V_2}{V_1}k_{31D} \\ \frac{V_1}{V_3}k_{12D} + \frac{V_1}{V_2}k_{13D}t_{23} & -k_{21D} & (k_{21D} - k_{31D} - k_{eD3})t_{23} \\ \frac{V_1}{V_2}k_{13D} & 0 & -(k_{31D} + k_{eD3}) \end{pmatrix}. \quad (48)$$

Now we impose

$$k'_{eD3} := -a'_{33} - \frac{V_1}{V_2}a'_{13} = 0, \quad (49)$$

from which we get  $t_{23} = -(V_2/V_3)(k_{eD3}/k_{21D})$ . After putting this last piece into  $A'$ , we get  $k'_{eD1}$  from

$$\begin{aligned} k'_{eD1} &= -a'_{11} - \frac{V_3}{V_1}a'_{21} - \frac{V_2}{V_1}a'_{31} \\ &= k_{eD1} - \frac{k_{13D} \cdot k_{eD3}}{k_{21D}}. \end{aligned} \quad (50)$$

Thus  $CL' = k'_{eD1} \cdot V_1$ , with  $k'_{eD1}$  given by (50). And finally we get  $D_{\text{tot,avg1}} = \text{Dose}/(CL' \cdot \tau)$ , and  $D_{\text{tot,avg3}} = B \cdot D_{\text{tot,avg1}}$ .

*Remark:* In the similarity transform, we measure  $D_1$  and  $D_3$ , which is indicated by  $C$ . As a result of imposing  $C' = C$ , the original model and the transformed model output the same values for these variables.  $D'_2$ , however, differs from  $D_2$ .

## Study Highlights

**What is the current knowledge on the topic? XYZ**

**What question did this study address? XYZ**

**What this study adds to our knowledge? XYZ**

**How might this change drug discovery, development and/or therapeutics? XYZ**

## Acknowledgements

The authors would like to thank XYZ for many helpful discussions.

## Conflict of Interest

Andrew Stein is employed by Novartis Institute for BioMedical Research

## Author Contributions

XYZ analyzed the data, XYZ performed the research, XYZ wrote the manuscript.

## References

- [1] W. Wang and H. Zhou, “Pharmacological considerations for predicting pk/pd at the site of action for therapeutic proteins,” *Drug Discovery Today: Technologies*, vol. 21, pp. 35–39, 2016.

- [2] A. Lindauer, C. Valiathan, K. Mehta, V. Sriram, R. de Greef, J. Elassaiss-Schaap, and D. de Alwis, “Translational pharmacokinetic/pharmacodynamic modeling of tumor growth inhibition supports dose-range selection of the anti-pd-1 antibody pembrolizumab,” *CPT: pharmacometrics & systems pharmacology*, vol. 6, no. 1, pp. 11–20, 2017.
- [3] J.-M. Boeynaems, J. E. Dumont, *et al.*, *Outlines of receptor theory*. Elsevier/North-Holland Biomedical Press, 1980.
- [4] A. Stein and R. Ramakrishna, “Afir: A dimensionless potency metric for characterizing the activity of monoclonal antibodies,” *CPT: pharmacometrics & systems pharmacology*, vol. 6, no. 4, pp. 258–266, 2017.
- [5] D. E. Mager and W. J. Jusko, “General pharmacokinetic model for drugs exhibiting target-mediated drug disposition,” *Journal of pharmacokinetics and pharmacodynamics*, vol. 28, no. 6, pp. 507–532, 2001.

## 8 Figures and Tables

There is a limit of 6 tables and figures in the paper.

Drug	Trastuzumab	Pembrolizumab	Atezolizumab	Bevacizumab
Target Type	Membrane-Bound	Membrane-Bound	Membrane-Bound	Soluble
Target	HER2	PD-1	PD-L1	VEGF
Baseline Target (nM)	X	Y	Z	A
Other info?				

Table 1: Summary of drugs in this analysis. Listing all the parameters is probably a bit nuts. I’d rather refer the reader to teh spreadsheet and also in the appendix or supplementary material we can give more information.

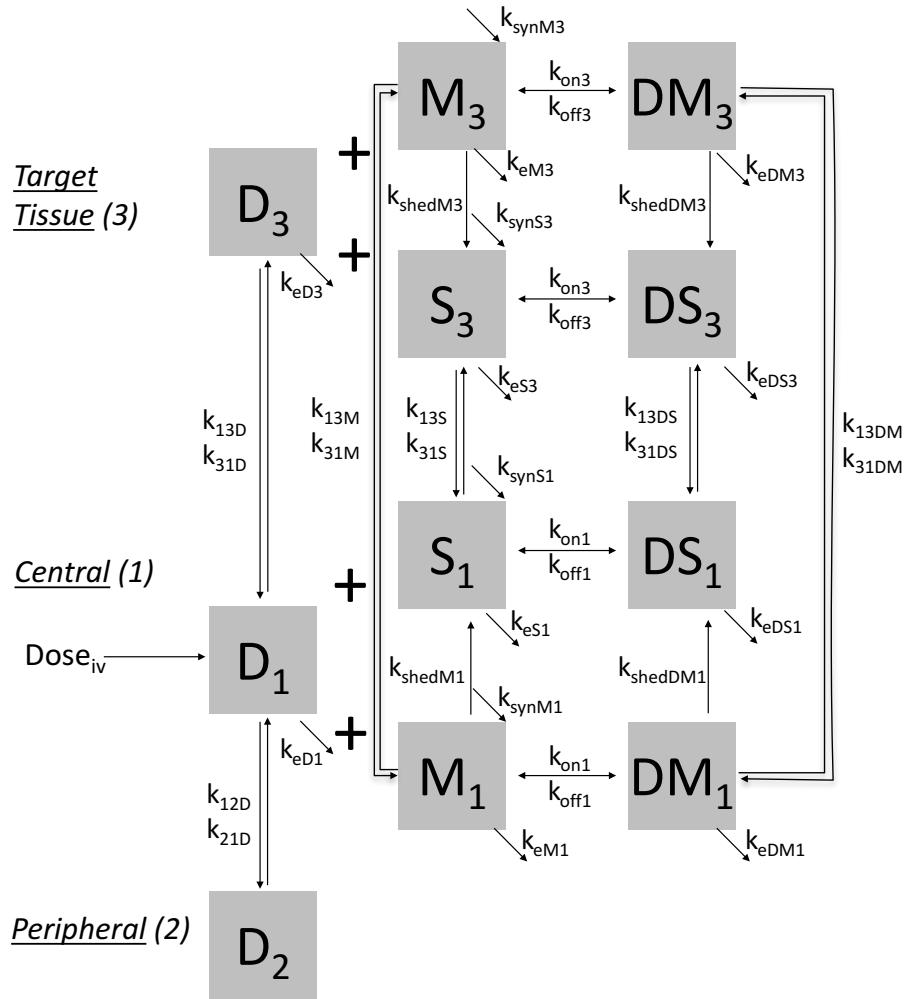


Figure 1: The extended target mediated drug disposition model. Vertical arrows represent distribution, horizontal arrows represent dosing and binding, and diagonal arrows represent synthesis and elimination.

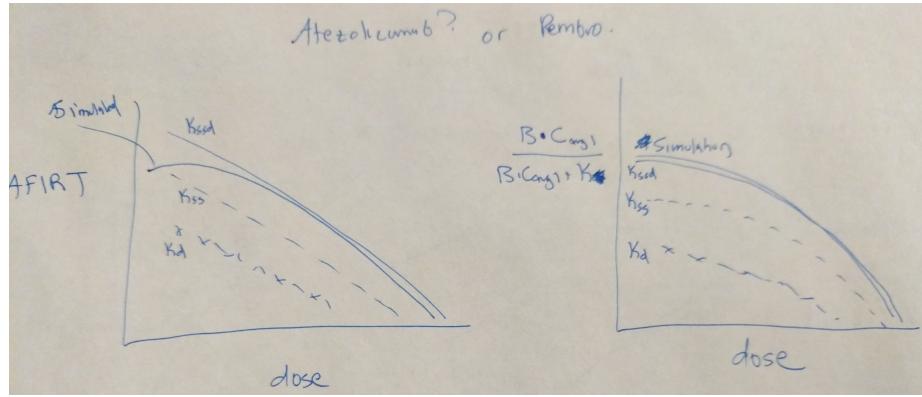


Figure 2: Here we show  $K_d$ ,  $K_{ss}$ ,  $K_{ssd}$  and that  $K_{ssd}$  is superior for describing the data. Might want to show for all four drugs and that  $K_{ssd}$  will be superior for atezo and pembro, though maybe all will be terrible for herceptin.

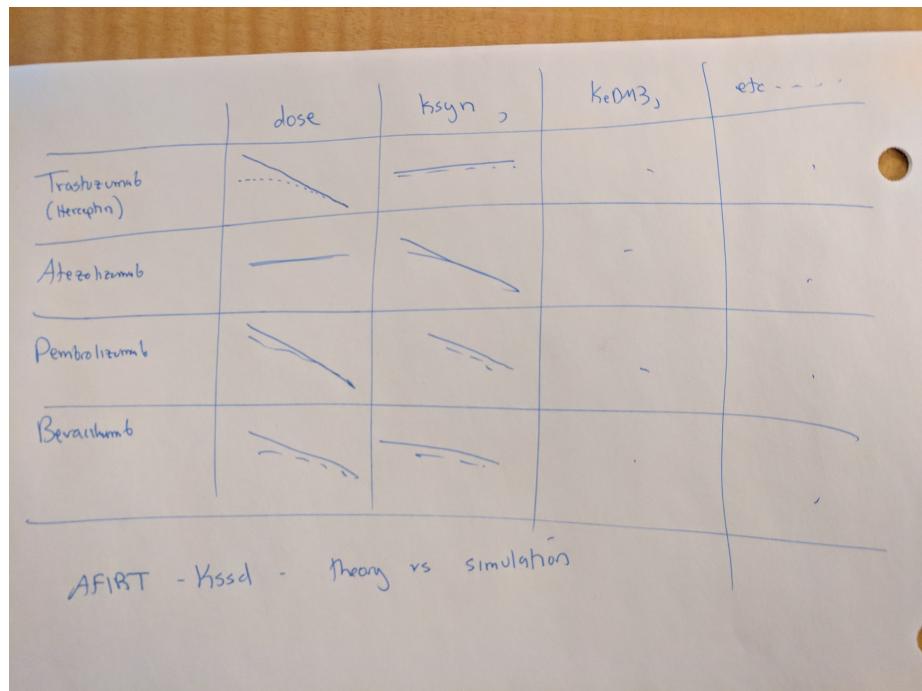


Figure 3: Sensitivity analysis that Sameed is currently working on (building off Hongshan's initial code). This will show the accuracy of the AFIRT (or lack thereof) over a wide range of scenarios

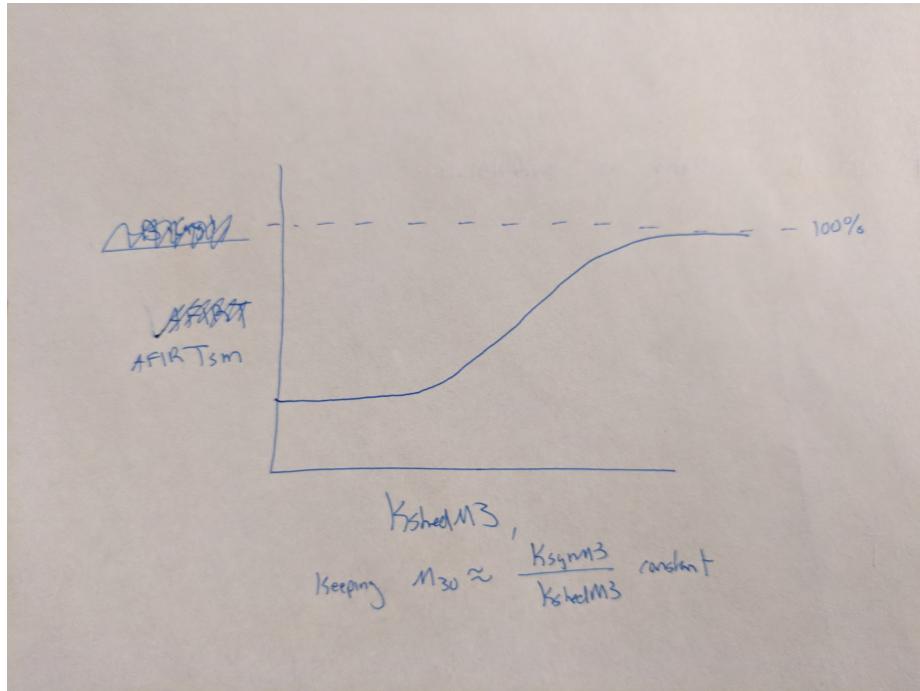


Figure 4: This will show that if the shedding is super fast, inhibiting the target is impossible. This can also I think readily be seen from the Kssd equation.

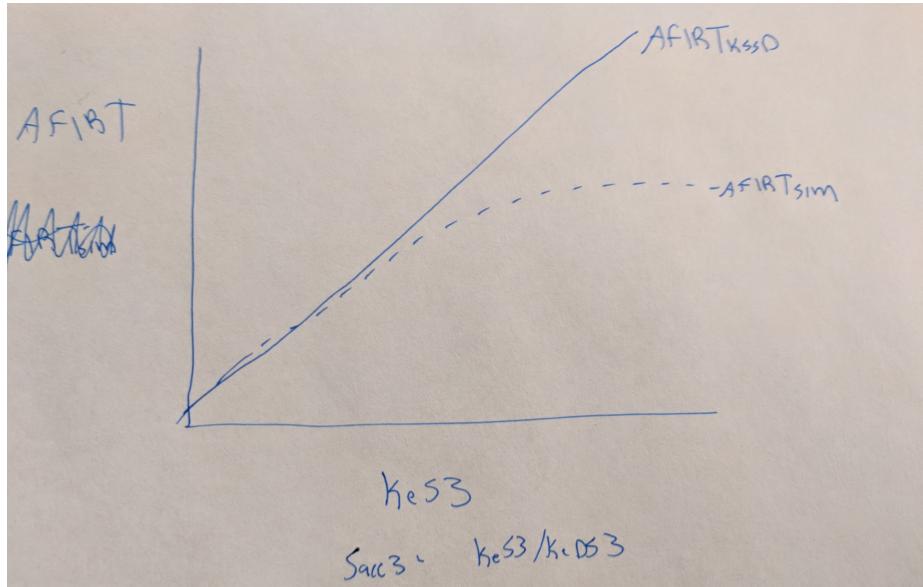


Figure 5: This will show that understanding the accumulation of the target in the tissue is critical. But this is often not measured.

WE MIGHT WANT ONE MORE FIGURE LOOKING AT THE ACCURACY OF  $K_{ssd}$  AS THE DISTRIBUTION BECOMES SLOW OR FAST.