

Single IMU-Based Multi Segment Motion Analysis and Prediction

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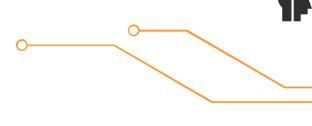


Achievements

 [ICDATE2023] Lower Limb Gait Estimation Using Foot Motion and Neural Network (Published)







Introduction



Background

- Human Gait and Accurately Estimating Joint Motion is crucial in the field of rehabilitation and motion analysis.
- Traditional methods of gait analysis include motion tracking systems that capture joint angles and provide insights to movement disorders - prove to be complex, expensive and require extensive setup [1]
- Abnormal Gait is the result of injuries that affect joints in the body that further affect the cyclic patterns that emerges [6].



Literature Review

Author	Methodology	Input	Output	Results
Mundt et al. [2]	IMU data fed to FNN	IMU Acceleration	Joint Angles and Moments	Joint Angle ρ = 0.85 RMSE < 4.8 Joint Moment ρ = 0.95 nRMSE < 13%
Mundt et al. [3]	IMU data fed to ANN (MLP, LSTM, <mark>CNN</mark>)	IMU Acceleration	Joint Angles and Moments	Joint Angle ρ = 0.832 Joint Moment ρ = 0.96
Senanayake et al. [4]	IMU data fed into DNN (GAN)	IMU Inverse Kinematics	Joint Angles	IK ρ < 0.05 IMU ρ < 0.001
Komaris et al. [5]	IMU data fed to ANN	Acceleration	Running Speeds and GRFs	Running Speed ρ = 0.23 RMSE vertical = 0.146
Chin-Hsien et al. [6]	IMU data fed into DNN	IMU Inverse Kinematics	Parkinson's Stage Condition	Advanced Stage Detection accuracy: 92.72% Early Stage Detection accuracy: 99.67%

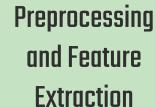
Hypothesis

- In Human Gait there is an evident relationship between the shank and the thigh segment in terms of biomechanics and the cyclic patterns of gait [6].
- This relationship between the kinematic chain of shank and thigh will be investigated and used to estimate values of thigh angular velocities from data collected from shank

- Research Gap Minimal approaches that can provide accurate joint motion estimation while being minimally invasive and cost-effective
- Novelty Collect subject data estimating thigh angular velocities from shank angular velocity data to see progression of injury

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Joint Estimation using Machine Learning



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Required relevant features extracted from sensors to represent joint

Joint Estimation

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Provide quantitative estimations of thigh angular velocities for analysis

Data Collection

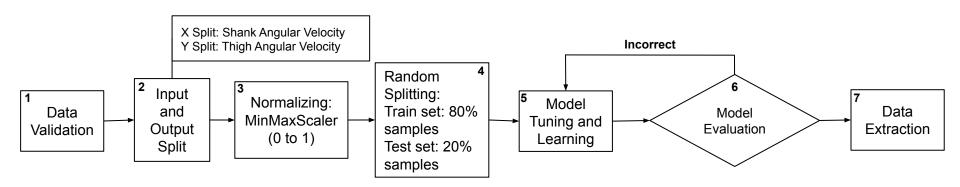
INITIAL STAGE
Data collected from
wearable sensors

Use suitable algorithms to train model

Machine Learning

Model Training

Gait Angular Velocity Estimation Flow Diagram

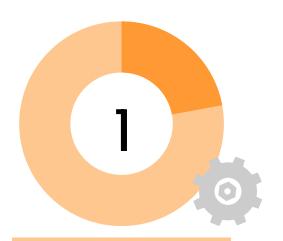


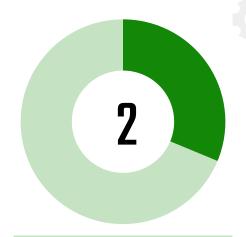


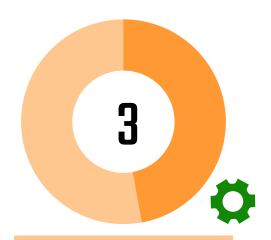




Objectives







Develop dataset using IMU sensors to capture angular velocity data during gait

Create machine learning model with at least 80% pearson correlation for estimation of thigh angular velocity using data obtained from a single IMU sensor attached to the shank

Develop IMU sensor system for the collection of angular velocity data from shank and thigh segments





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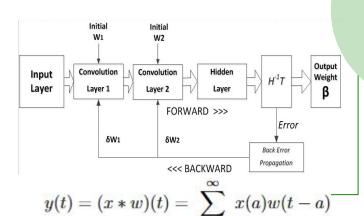
Methodology



Using Deep Learning -CNN

Introduction

- Creates a linear stack of layers in deep learning models
- Easily learn dynamics of joint movements through *feature* selection [3]



Convolutional Neural Network

Training

- Feeding integrated sensor data (80%) + optimize model parameters
- Integrated data divided into training and validation sets
- Use of backpropagation

- Training on evaluation set consisting of data the model has not seen (20%)
- CNN generates predicted values

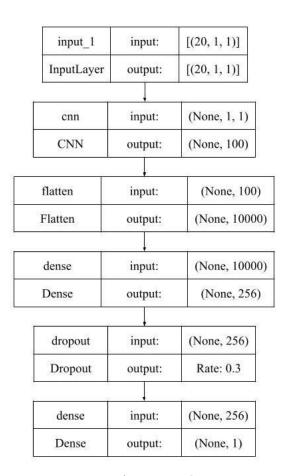
Evaluation/Validation

The CNN Model - Layers

- 1. **Input Layer** has a shape of [20, 1, 1]. This shape indicates model is designed to handle time-series data with 20 time steps and one feature.
- 2. Convolutional Layer is the first hidden layer. It is 1D convolutional layer with 128 filters [for time series data where data proximity matters]. Scans input data to identify important patterns, with each filter looking for different patterns. The ReLU activation function is used to introduce non-linearity into the model.
- 3. **Flatten Layer** takes output of convolutional layer and transforms it into a 1D tensor. Necessary as subsequent Dense layers require a 1D input and not the multidimensional output of the convolutional layer.

4. Dense Layers

- First Dense layer with 256 units as an output layer. Processes the flattened data to make predictions.
- Dropout layer with a rate of 0.3 is added to prevent overfitting by randomly disabling a portion of neurons during training.
- Final Dense layer with 1 unit provides the model's output, the estimated thigh angular velocity.



Layer Architecture of CNN

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The CNN Model - Parameters

1. Optimizer

- Adam Optimizer used is a optimization algorithm in deep learning. Adapts learning rates for each parameter individually - leads to faster convergence + better performance.
- A learning rate of 0.001 indicates the step size at which the model's weights are updated during training.
- Smaller learning rate can result in slower training but helps model converge more effectively
- Larger learning rate may speed up training but could lead to overshooting optimal weights.

1. Hyperparameters

- Batch Size: Determines how many data samples processed in each forward/backward pass during training. Smaller batch (32-128) size-more stable training but slower. Larger batch (>256) size-speed up training but less stable.
- Number of Epochs: An epoch is one complete pass through the entire training dataset. Total number specifies how many times model sees entire dataset depends on dataset and convergence of model. Early stopping also implemented where training stops when performance on validation set no longer improves.

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The CNN Model - Parameters

3. Loss Function and Metrics

 Mean Squared Error (MSE) is a loss function for regression tasks. Calculates average of squared differences between model's predictions and actual target values. Lower MSE values indicate better performance.

 $MSE = \frac{1}{N} \sum_{i=1}^{N} (y_i - \hat{y}_i)^2$

- Mean Absolute Error (MAE) is a metric that calculates the average of the absolute differences between predictions and actual values. Less sensitive to outliers compared to MSE.

$$MAE = \frac{1}{n} \sum_{i=1}^{n} |Y_i - \hat{Y}_i|$$

- Root Mean Squared Error (RMSE) takes into account relative error and provide insights into the model's ability to estimate thigh angular velocity.

RMSE =
$$\sqrt{\frac{1}{N} \sum_{i=1}^{N} (y_i - \hat{y}_i)^2}$$

- Correlation Coefficient (p) measures linear relationship between predicted and actual values. Ranges from -1 to 1:1 indicating perfect positive linear relationship, -1 indicating perfect negative linear relationship. 0 means no linear relationship.

$$\rho = \frac{\sum_{i=1}^{n} (x_i - \bar{x})(y_i - \bar{y})}{\sqrt{\sum_{i=1}^{n} (x_i - \bar{x})^2} \sqrt{\sum_{i=1}^{n} (y_i - \bar{y})^2}}$$



Obtaining the Dataset

Hardware

- ESP32 Microcontroller serves as central processing units for data collection
- MPU6050 Module employed to measure and record angular velocity values of shank and thigh







Data Collection + Recording

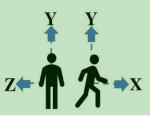
- 10 subjects selected (5M/5F):
- Subjects wear sensor equipped devices on shank and thigh

Age (years)	21.6±0.92
Weight (kg)	63.2±11.79
Height (cm)	164.8土7.57

- Angular Velocity Collected: Gait motion and apparent analysis
- Z-Axis for Shank and Y-Axis for Thigh [7]



- Normal Gait Data Collected
- 1 kg Sandbag simulate knee injury-Abnormal Gait Data Collected
- Data stored in time series datasets



Software

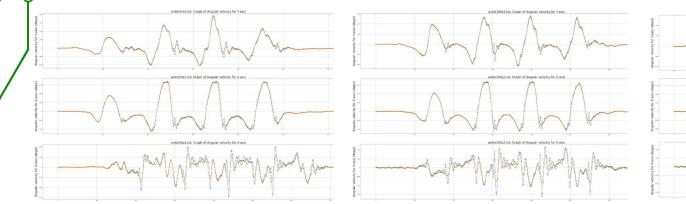
- To facilitate data transmission and recording
- Bluetooth technology to establish wireless connection between hardware and device
- Python Script to generate appropriate data format
- Received data is processed / stored as .CSV file

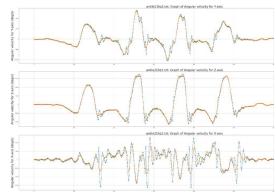


Data Preprocessing and Training

Filter Selection

- Filters are essential for noise reduction and ensuring relevant information is captured.
- Experimented with multiple filter frequencies: 5Hz, 10Hz, and 21Hz. These frequencies were applied to raw data collection to preprocess for subsequent modeling.
- Data filtered at 10Hz emerged as best choice, delivering best results for model.





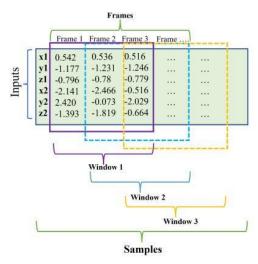
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Data Preprocessing and Training

Windowing

- Windowing involves dividing time-series data into small segments. Each segment, or "window," captures local patterns within the data, allowing the model to analyze sequences effectively [8].
- Model considers last 20 time steps to predict next value, creating input-output pairs for neural network.
- Improves understandability and complex time-series data by enabling model to focus on relevant local patterns.



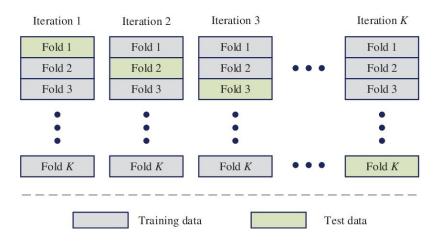


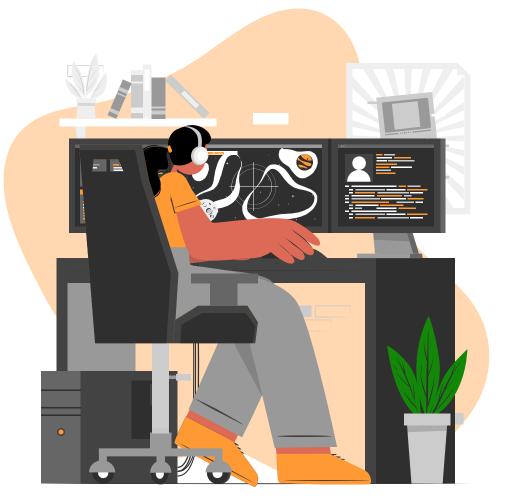


Data Preprocessing and Training

K-Fold Validation

- Robust technique used to assess performance of machine learning models. Partitions dataset into "k" subsets, trains the model on "k-1" subsets, and tests on remaining subset [9].
- Implemented 5-fold cross-validation using scikit-learn. Each fold trained on different portion of data.
- Helps detect overfitting, where model performs well on training data but poorly on new data. By assessing performance on multiple subsets, it provides insights into model's ability to generalize to unseen data.



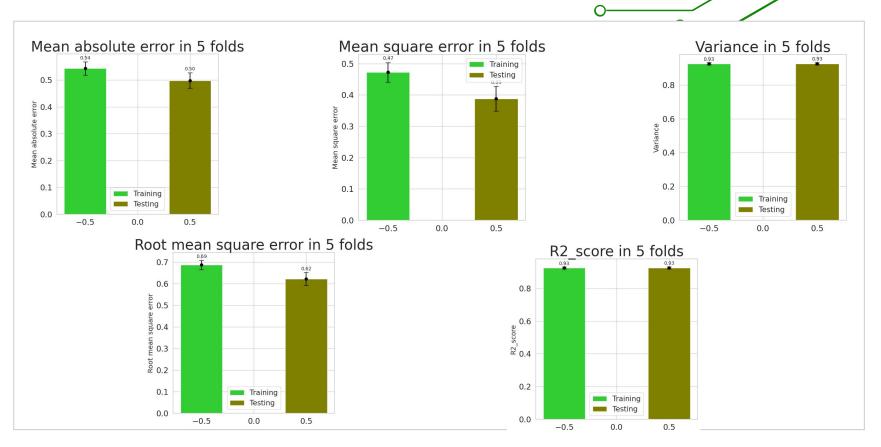




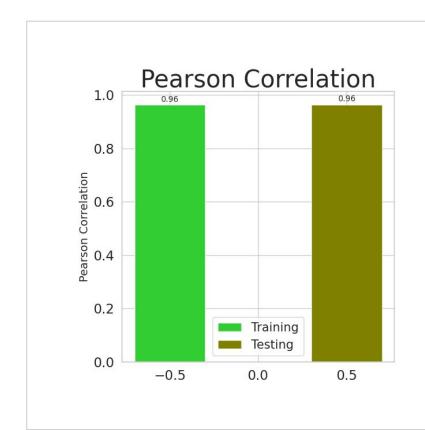
Results and Discussion

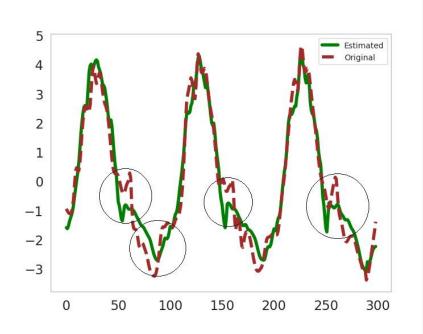


Results - Normal Thigh Angular Velocity Estimation



Results - Normal Thigh Angular Velocity Estimation (cont.)

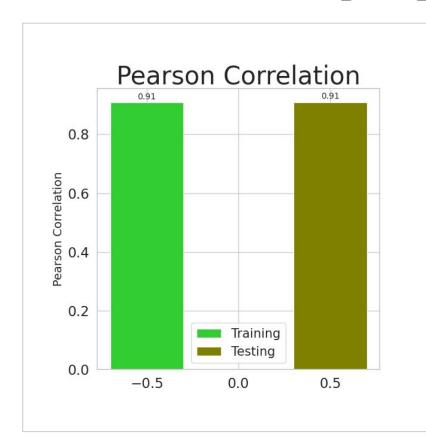


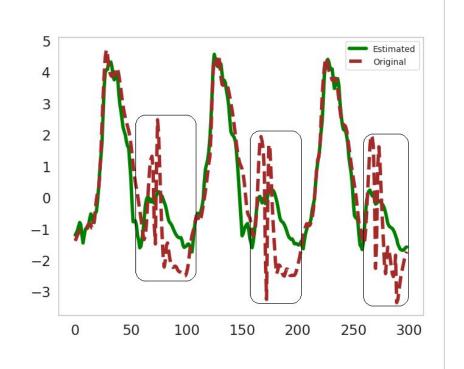


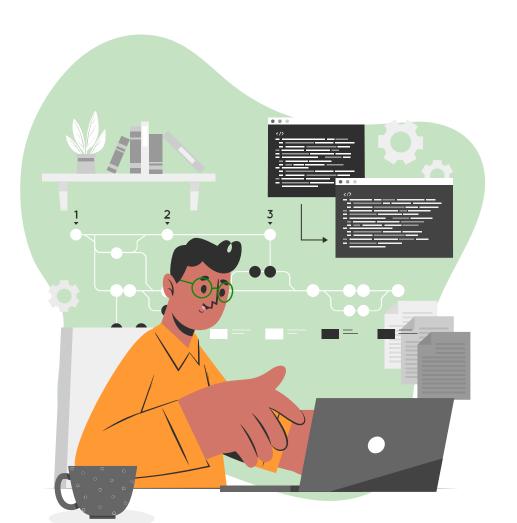
Results - Abnormal Thigh Angular Velocity Estimation



Results - Abnormal Thigh Angular Velocity Estimation (cont.)







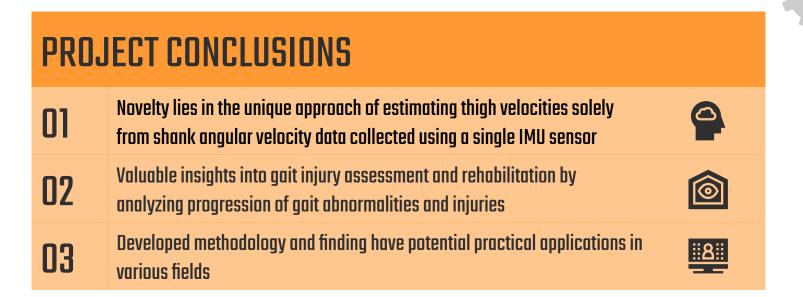


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Conclusion and Future Works

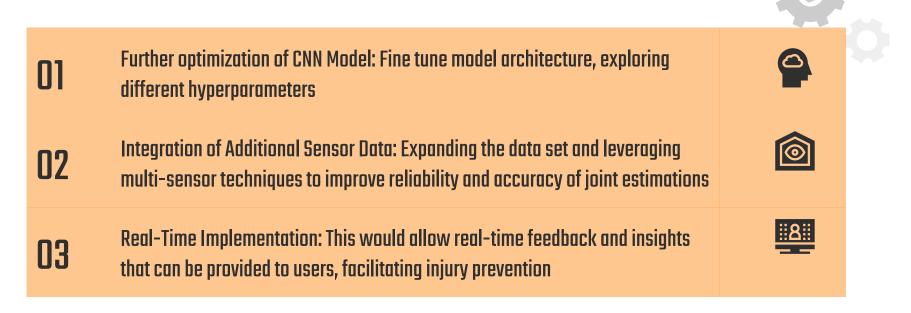


Conclusion





Future Works



References

- S. Veeraragavan, A. Gopalai, D. Gouwanda, and S. Ahmad, "Parkinson's disease diagnosis and severity assessment using ground reaction forces and neural networks," Frontiers in Physiology, vol. 11, p. 587 057, 2020. doi: 10.3389/fphys.2020.587057.
- 2. M. Mundt, W. R. Johnson, W. Potthast, B. Markert, A. Mian, and J. Alderson, "A comparison of three neural network approaches for estimating joint angles and moments from inertial measurement units," Sensors, vol. 21, no. 13, p. 4535, 2021. doi: 10.3390/s21134535.
- 3. M. Mundt, A. Koeppe, S. David, et al., "Estimation of gait mechanics based on simulated and measured imu data using an artificial neural network," Frontiers in Bioengineering and Biotechnology, vol. 8, p. 41, 2020. doi: 10.3389/fbioe.2020.00041.
- 4. D. Senanayake, S. Halgamuge, and D. C. Ackland, "Real-time conversion of inertial measurement unit data to ankle joint angles using deep neural networks," Journal of Biomechanics, vol. 125, p. 110 552, 2021, issn: 0021- 9290. doi: 10.1016/j.jbiomech.2021.110552.
- 5. D. .-. Komaris and et al., "Predicting three-dimensional ground reaction forces in running by using artificial neural networks and lower body kinematics," IEEE Access, vol. 7, pp. 156 779–156 786, 2019. doi: 10 . 1109 / ACCESS.2019.2949699.
- 6. C.-H. Lin, F.-C. Wang, T.-Y. Kuo, P.-W. Huang, S.-F. Chen, and L.-C. Fu, "Early detection of parkinson's disease by neural network models," IEEE Access, vol. 10, pp. 19 033–19 044, 2022. doi: 10 . 1109 / ACCESS . 2022 . 3150774.

References

- 7. Hirano, S., Uchida, H., Nakatoh, Y., Li, Y. (2023). Estimation of Gait Conditions Using Acceleration and Angular Velocity Sensors. In: Tareq Ahram and Redha Taiar (eds) Human Interaction & Emerging Technologies (IHIET 2023): Artificial Intelligence & Future Applications. AHFE (2023) International Conference. AHFE Open Access, vol O. AHFE International, USA. http://doi.org/10.54941/ahfe1004096
- 8. M. Jaen-Vargas, K. Reyes Leiva, F. Fernandes, et al., "Effects of sliding window variation in the performance of acceleration-based human activity recognition using deep learning models," PeerJ Comput Sci, vol. 8, e1052, Aug. 2022. doi:10.7717/peerj-cs.1052.
- 9. Q. Ren, M. Li, and S. Han, "Tectonic discrimination of olivine in basalt using data mining techniques based on major elements: A comparative study from multiple perspectives," Big Earth Data, vol. 3, pp. 1–18, Feb. 2019. doi: 10.1080/20964471.2019.1572452. 89



THANKS!

DO YOU HAVE ANY QUESTIONS?

