



Contents lists available at SciVerse ScienceDirect

Journal of the Mechanics and Physics of Solids

journal homepage: www.elsevier.com/locate/jmps



On the mechanics of continua with boundary energies and growing surfaces

Areti Papastavrou^a, Paul Steinmann^b, Ellen Kuhl^{c,d,e,*}

^a Department of Electrical Engineering and Computer Sciences, Hochschule für Angewandte Wissenschaften Ingolstadt, 85049 Ingolstadt, Germany

^b Chair of Applied Mechanics, Department of Mechanical Engineering, University of Erlangen/Nuremberg, 91058 Erlangen, Germany

^c Department of Mechanical Engineering, Stanford University, Stanford, CA 94305, USA

^d Department of Bioengineering, Stanford University, Stanford, CA 94305, USA

^e Department of Cardiothoracic Surgery, Stanford University, Stanford, CA 94305, USA

ARTICLE INFO

Article history:

Received 5 September 2012

Received in revised form

23 December 2012

Accepted 22 January 2013

Available online 8 February 2013

Keywords:

Boundary energy

Growth

Finite elements

Airway wall remodeling

Thin films

ABSTRACT

Many biological systems are coated by thin films for protection, selective absorption, or transmembrane transport. A typical example is the mucous membrane covering the airways, the esophagus, and the intestine. Biological surfaces typically display a distinct mechanical behavior from the bulk; in particular, they may grow at different rates. Growth, morphological instabilities, and buckling of biological surfaces have been studied intensely by approximating the surface as a layer of finite thickness; however, growth has never been attributed to the surface itself. Here, we establish a theory of continua with boundary energies and growing surfaces of zero thickness in which the surface is equipped with its own potential energy and is allowed to grow independently of the bulk. In complete analogy to the kinematic equations, the balance equations, and the constitutive equations of a growing solid body, we derive the governing equations for a growing surface. We illustrate their spatial discretization using the finite element method, and discuss their consistent algorithmic linearization. To demonstrate the conceptual differences between volume and surface growth, we simulate the constrained growth of the inner layer of a cylindrical tube. Our novel approach toward continua with growing surfaces is capable of predicting extreme growth of the inner cylindrical surface, which more than doubles its initial area. The underlying algorithmic framework is robust and stable; it allows to predict morphological changes due to surface growth during the onset of buckling and beyond. The modeling of surface growth has immediate biomedical applications in the diagnosis and treatment of asthma, gastritis, obstructive sleep apnoea, and tumor invasion. Beyond biomedical applications, the scientific understanding of growth-induced morphological instabilities and surface wrinkling has important implications in material sciences, manufacturing, and microfabrication, with applications in soft lithography, metrology, and flexible electronics.

© 2013 Elsevier Ltd. All rights reserved.

* Corresponding author at: Department of Mechanical Engineering, Stanford University, 496 Lomita Mall, Stanford, CA 94305, USA. Tel.: +1 650 450 0855; fax: +1 650 725 1587.

E-mail addresses: aretipapastavrou@haw-ingolstadt.de (A. Papastavrou), paul.steinmann@itm.uni-erlangen.de (P. Steinmann), ekuhl@stanford.edu (E. Kuhl).

URL: <http://biomechanics.stanford.edu> (E. Kuhl).

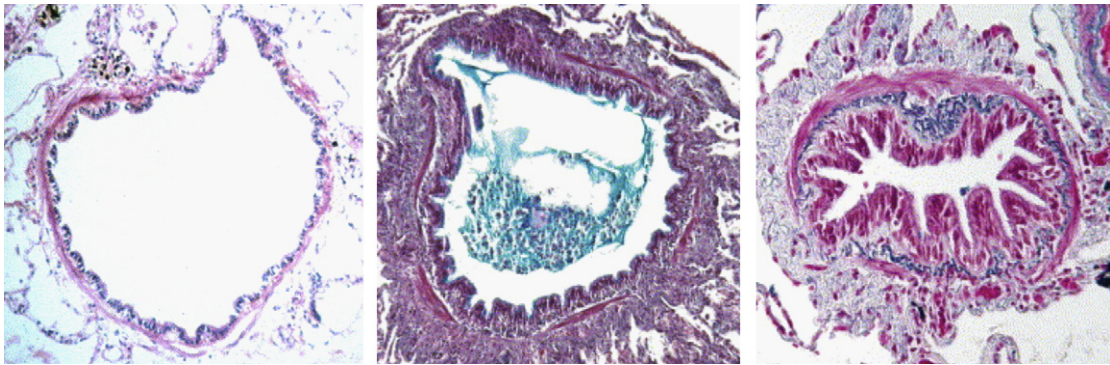


Fig. 1. Chronic airway wall remodeling and characteristic structural changes. Normal small airway (left). Acutely inflamed airway with thickened airway wall, in which the lumen is partly filled with an inflammatory exudate of mucus and cells (middle). Chronically obstructed airway with increased deposition of collagen and thickened smooth muscle layer, which restricts normal enlargement of the lumen and unfolding of the epithelial lining during inflation (right). Reprinted with permission from Hogg (2004).

1. Introduction

Just like skin covers and protects the outer surface of our body, the mucous membrane covers and protects our inner body surfaces. The mucous membrane is a thin, moist layers of epithelial cells, which lines the air–organ interface of our respiratory, digestive, and urogenital tracts, and of our mouth and nose. It is attached to a soft submucosal layer supported by an outermost layer of smooth muscle cells. Surface wrinkling of the mucous membrane is critical for healthy biological function, and abnormalities in wrinkling patterns are a classical hallmark of disease (Wiggs et al., 1997). A typical example is severe asthma, a chronic disease of the respiratory system, for which there is currently no cure. As illustrated in Fig. 1, during chronic asthma, the airway wall undergoes an irreversible structural remodeling, associated with an increased deposition of collagen, a permanent thickening of the smooth muscle layer, growth of the mucous membrane, and mucosal folding (Hogg, 2004). Collectively, these changes induce an excessive airway wall narrowing, resulting in progressively reduced lung function (Davies et al., 2003).

1.1. The mechanical origin of morphological instabilities

The mechanical origin of mucosal folding in healthy and asthmatic airways was first studied more than a decade ago using an analytical linear elastic model (Wiggs et al., 1997). Linear stability analysis of bilayered tubes can explain to which extent the ratio between thicknesses and elastic moduli of the mucosal and submucosal layers dictates the morphology of surface buckling (Li et al., 2011; Moulton and Goriely, 2011). A recent study confirmed the hypothesis that the wrinkling mode, the number of folds, is highly sensitive to the thickness ratio of these two layers, with more folds in the thin mucosal layer of the airway and fewer folds in the thick mucosal layer of the esophagus (Li et al., 2011). Beyond mucosal folding during airway narrowing in asthma (Wiggs et al., 1997 and surface wrinkling in the esophagus (Li et al., 2011), morphological instabilities have been thoroughly investigated in the context of buckling during crypt formation in the intestinal wall (Nelson et al., 2011), mucosal folding in the gastrointestinal tract (Liao et al., 2007), lumen narrowing during chronic obstructive pulmonary disease (Hogg, 2004), ruffle formation in cyclically loaded arteries (Lee and Chien, 1978), and buckling in the pharynx during obstructive sleep apnoea (Kairaitis, 2012). In addition to these common diseases, understanding the morphogenesis and origin of shape has been identified as one of the key challenges in developmental biology (Wyczalkowski et al., 2012; Xu et al., 2010).

While the onset of mucosal buckling was initially attributed to an elevated external pressure, current hypotheses suggest that physiological and pathological thickening of the individual layers, as illustrated in Fig. 1, might play a critical role in the generation of morphological instabilities (Pare et al., 2007; Moulton and Goriely, 2011). A recent model experiment of a cultured growing epithelial monolayer on a thin elastic substrate confirmed that growth of biological surfaces can, indeed, induce significant substrate buckling (Nelson et al., 2011). Another model experiment of a swelling polyacrylamide gel displayed similar buckling phenomena at the gel–water interface (Dervaux and Ben Amar, 2011). Only now, we are beginning to recognize the striking similarities between growing biological tissues and swelling gels, which display almost identical surface phenomena. These findings initiated a thorough mathematical analysis of crease formation in growing soft matter (Jin et al., 2011) and of surface wrinkling in core-shell soft cylinders (Cao et al., 2012) using continuum models of isotropic volumetric growth. An excellent recent overview article illustrates various phenomena of morphological instabilities including applications beyond biological systems, such as soft lithography, metrology, and flexible electronics (Li et al., 2012).

1.2. Continuum modeling of mechanically induced biological growth

Conceptually, volumetric growth models can be classified into two categories, models of mechanically induced biological growth and models of growth-induced mechanical instabilities. The first pioneering continuum model for

mechanically induced biological growth was proposed almost two decades ago (Rodriguez et al., 1994). Since then, it has been widely adopted to model muscle growth (Taber, 1995; Zöllner et al., 2012b), vascular growth (Himpel et al., 2005; Taber and Humphrey, 2001), skin growth (Bugan Zatepole et al., 2012; Socci et al., 2007), and cardiac growth (Göktepe et al., 2010; Kroon et al., 2009) in response to elevated stresses or strains. Initially, these models were merely analytical (Epstein and Maugin, 2000; Garikipati, 2009), for example focussing on volume growth of idealized rotationally symmetric cylindrical tubes (Taber and Humphrey, 2001; Vandiver and Goriely, 2009). Now, computational growth models allow us to simulate growth in more realistic, fully three-dimensional, subject-specific geometries (Kuhl et al., 2007; Zöllner et al., 2012a). While the first generation of growth models was rather phenomenological and isotropic in nature (Ambrosi and Mollica, 2002; Kroon et al., 2009), the current trend goes toward incorporating the underlying mechanobiology (Zöllner et al., 2012) and the microstructural origin of growth (Göktepe et al., 2010). Depending on the particular tissue architecture, microstructurally motivated models are therefore unusually transversely isotropic (Rausch et al., 2011; Zöllner et al., 2012b), orthotropic (Göktepe et al., 2010), or generally anisotropic (Menzel, 2005; Tsamis et al., 2012). Various different biomedical applications of mechanically induced growth are summarized comprehensively in two recent overview articles (Ambrosi et al., 2011; Menzel and Kuhl, 2012).

1.3. Continuum modeling of growth-induced mechanical instabilities

The first continuum model for growth-induced mechanical instabilities was proposed a decade ago to study tumor growth in confined geometries (Ambrosi and Mollica, 2002). In the context of surface layer folding, the problem we are interested in here, recent studies have addressed circumferential buckling instabilities inside a growing cylindrical tube (Li et al., 2011; Moulton and Goriely, 2011). Again, anisotropic models have been proposed to allow for a more sophisticated analysis using independent growth multipliers in the circumferential and radial directions (McMahon and Goriely, 2010; Moulton and Goriely, 2011). These models attribute buckling to the progression of growth, whereas other studies report buckling instabilities as a result of cyclic pressure changes (Lee and Chien, 1978) and mechanical unloading (Buganza Tepole et al., 2011). While mechanical instabilities have been investigated intensely in growing solids, the interplay between growing surfaces and morphological instabilities remains severely understudied (Goriely and BenAmar, 2005). Since growing surfaces may undergo finite deformations, analytical solutions are usually either unavailable or incredibly complex, and only a handful of mathematical models exist to model a growing surface by means of nonlinear plate (Dervaux et al., 2009) or shell (Ben Amar and Goriely, 2005) theories. Using shell theories of surface growth, a recent study has found that growth of biological membranes does not necessarily have to be detrimental: In some diseases such as mitral valve leakage, an adaptive surface growth of more than 30% has been reported as a compensatory mechanism to chronically reduce mitral valve insufficiency and deleterious backflow (Rausch et al., 2012). Here, we adopt the kinematical framework of growing biological surfaces; however, rather than allowing the surface to move freely, we attach it kinematically to the underlying solid, but equip it with its own potential energy.

1.4. Continuum modeling of material surfaces

The concept of surface energies is by no means new; in fact it has first been recognized more than two centuries ago, formalized through the famous Young Laplace equation (Laplace, 1805; Young, 1805). Relating the pressure difference across a fluid surface to surface tension and mean curvature, the Young Laplace equation is known to explain a variety of different phenomena ranging from minimal surfaces, soap bubbles, and capillary pressure to cardiovascular and respiratory physiology (Suo, 1997). More than three decades ago, the familiar concept of scalar-valued surface tension was generalized to the tensorial notion of surface stress in the first continuum theory of elastic material surfaces (Gurtin and Murdoch, 1975). Since then, the concept of material surfaces has gained increasing popularity in crystallography (Leo and Sekerka, 1989), phase transformation (Leo and Sekerka, 1989; Simha and Bhattacharya, 1998), mineralogy (Kuhl and Schmid, 2007), micro- and nanofabrication, and soft lithography; broadly speaking, whenever the surface displays distinct characteristic properties (Gurtin and Struthers, 1990; Steinmann, 2008). Although propagations of internal surfaces (Simha and Bhattacharya, 2000) and morphological surface instabilities (Leo and Sekerka, 1989) are widely studied in metallurgy, material sciences, and mechanics today, the computational modeling of surfaces equipped with their own energies is still in its infancy. For fluids, a few finite element approaches exist to simulate droplets and free surfaces with scalar-valued surface tension (Saksono and Peric, 2006). For solids, however, a generic finite element approach toward elastic surfaces with tensorial surface stresses has only been proposed very recently (Javili and Steinmann, 2009). Conceptually speaking, this approach treats the surface as a hyperelastic membrane of zero thickness glued to the underlying bulk. This concept is mathematically elegant and easily generalizable to anisotropic surfaces (Javili and Steinmann, 2010), thermomechanical surfaces (Javili and Steinmann, 2011) and surfaces with diffusion (McBride et al., 2011). Here, we adopt this framework and model the growing surface as a growing shell, kinematically constrained to move with the solid body, but equipped with its own potential energy.

1.5. Organization of this manuscript

The manuscript is organized as follows. In Sections 2, 3, and 4, we introduce the kinematic equations, the balance equations, and the constitutive equations for finite growth. In all three sections, we first illustrate growth of the solid body,

and then adopt the underlying concept to growth of the surface. In Section 5, we summarize the weak form of the governing equations and discretize it in space using a combination of volume elements for the volume terms and surface elements for the surface terms. In Section 6, we illustrate the features of our algorithm using the model problem of constrained growth in a cylindrical tube. We systematically compare a growing volume layer of finite thickness to a growing surface of zero thickness. In Section 7, we discuss the differences between volume and surface growth, before we close with a conclusion in Section 8.

2. Kinematics of growth

2.1. Kinematics of volume growth

Let $\mathcal{B}_0 \in \mathbb{R}^3$ denote the material placement of a continuum body with material particles $\mathbf{X} \in \mathcal{B}_0$. We denote the time domain by $\mathbb{T} = [0, T] \subset \mathbb{R}_+$ and consider the quasi-static case, for which time provides a history parameter to order the sequence of events. We introduce the orientation preserving map $\varphi : \mathcal{B}_0 \times T \rightarrow \mathbb{R}^3$ as the smooth motion of the material placement \mathbf{X} onto its spatial placement \mathbf{x} at any time $t \in \mathbb{T}$

$$\mathbf{x} = \varphi(\mathbf{X}, t), \quad (1)$$

and label the current placement of the body at time t as $\mathcal{B}_t = \varphi(\mathcal{B}_0)$, see Fig. 2. Here and in the sequel, the subscripts 0 and t designate material and spatial quantities. We further introduce the gradient, divergence, and material rate of any field $\{\circ\}(\mathbf{X}, t)$ as

$$\nabla\{\circ\} = \partial_{\mathbf{X}}\{\circ\}|_t, \quad \text{Div}\{\circ\} = \nabla\{\circ\} : \mathbf{I}, \quad D_t\{\circ\} = \partial_t\{\circ\}|_{\mathbf{X}}, \quad (2)$$

where \mathbf{I} is the material identity tensor, and $\{\circ\}|_t$ and $\{\circ\}|_{\mathbf{X}}$ indicate fixed temporal and spatial positions. Using the above definitions, we introduce the deformation gradient $\mathbf{F} : T\mathcal{B}_0 \rightarrow T\mathcal{B}_t$, which maps material line elements $d\mathbf{X} \in T\mathcal{B}_0$ onto spatial line elements $d\mathbf{x} \in T\mathcal{B}_t$ as $d\mathbf{x} = \mathbf{F} \cdot d\mathbf{X}$. To account for volumetric growth, we multiplicatively decompose the deformation gradient into an elastic part \mathbf{F}^e and a growth part \mathbf{F}^g (Rodriguez et al., 1994)

$$\mathbf{F} = \nabla\varphi \quad \text{with} \quad \mathbf{F} = \mathbf{F}^e \cdot \mathbf{F}^g. \quad (3)$$

In contrast to the deformation gradient \mathbf{F} , however, its individual contributions \mathbf{F}^e and \mathbf{F}^g can, in general, be incompatible (Lee, 1969). For notational convenience, we also introduce the inverses of these second order tensors as $\mathbf{f} = [\mathbf{F}]^{-1}$, $\mathbf{f}^e = [\mathbf{F}^e]^{-1}$, and $\mathbf{f}^g = [\mathbf{F}^g]^{-1}$. The Jacobian J of the deformation gradient \mathbf{F} relates material volume elements $dV_0 \in \mathcal{B}_0$ and spatial volume elements $dV_t \in \mathcal{B}_t$ as $dV_t = J dV_0$. Similar to the deformation gradient, we can decompose it multiplicatively into an elastic part J^e and a growth part J^g

$$J = \det(\mathbf{F}) > 0 \quad \text{with} \quad J = J^e J^g. \quad (4)$$

We can explicitly express the elastic Jacobian $J^e = \det(\mathbf{F}^e)$ and the growth Jacobian $J^g = \det(\mathbf{F}^g)$, where we introduce the following explicit representation in terms of the $I = 1, 2, 3$ covariant base vectors \mathbf{G}_I in $T\mathcal{B}_0$

$$\det(\mathbf{F}^g) = \frac{[\mathbf{F}^g \cdot \mathbf{G}_1] \cdot [[\mathbf{F}^g \cdot \mathbf{G}_2] \times [\mathbf{F}^g \cdot \mathbf{G}_3]]}{\mathbf{G}_1 \cdot [\mathbf{G}_2 \times \mathbf{G}_3]}. \quad (5)$$

Last, we introduce the right Cauchy Green tensor \mathbf{C} in the material configuration and its elastic counterpart \mathbf{C}^e in the intermediate configuration as characteristic deformation measures

$$\mathbf{C} = \mathbf{F}^t \cdot \mathbf{F} \quad \text{and} \quad \mathbf{C}^e = \mathbf{F}^{et} \cdot \mathbf{F}^e, \quad (6)$$

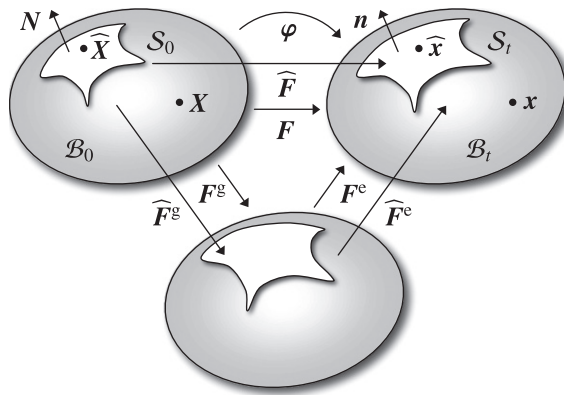


Fig. 2. Kinematics of material and spatial configurations \mathcal{B}_0 and \mathcal{B}_t of material body with material and spatial surfaces S_0 and S_t and multiplicative decomposition of the volume and surface deformation gradients $\mathbf{F} = \mathbf{F}^e \cdot \mathbf{F}^g$ and $\widehat{\mathbf{F}} = \widehat{\mathbf{F}}^e \cdot \widehat{\mathbf{F}}^g$ into elastic parts \mathbf{F}^e and $\widehat{\mathbf{F}}^e$ and growth parts \mathbf{F}^g and $\widehat{\mathbf{F}}^g$.

which are related through the identity $\mathbf{C}^e = [\mathbf{f}^g]^t \cdot \mathbf{C} \cdot \mathbf{f}^g$. With the above considerations, the pull back of the spatial velocity gradient \mathbf{I} to the intermediate configuration

$$\mathbf{I} = \mathbf{D}_t \mathbf{F} \cdot \mathbf{f} \quad \text{with} \quad \mathbf{f}^e \cdot \mathbf{I} \cdot \mathbf{F}^e = \mathbf{L}^e + \mathbf{L}^g, \quad (7)$$

obeys an additive decomposition into the elastic velocity gradient $\mathbf{L}^e = \mathbf{f}^e \cdot \mathbf{D}_t \mathbf{F}^e$ and the growth velocity gradient $\mathbf{L}^g = \mathbf{D}_t \mathbf{F}^g \cdot \mathbf{f}^g$.

2.2. Kinematics of surface growth

Let $S_0 = \partial B_0$ denote the surface of B_0 , assumed smooth, such that $\bar{B}_0 = B_0 \cup S_0$ is the closure of B_0 and S_0 . We label points on the surface of the reference configuration S_0 as $\hat{\mathbf{X}} = \mathbf{X}|_{S_0}$, and the unit outward normal to S_0 as \mathbf{N} , see Fig. 2. We can then introduce the surface deformation map $\hat{\phi} : S_0 \times T \rightarrow \mathbb{R}^3$ as the smooth motion of points on the surface of the material configuration $\hat{\mathbf{X}}$ onto points on the surface of the spatial configuration $\hat{\mathbf{x}} = \mathbf{x}|_{S_t}$ at any time $t \in T$ (Steinmann, 2008)

$$\hat{\mathbf{x}} = \hat{\phi}(\hat{\mathbf{X}}, t). \quad (8)$$

The above considerations implicitly assume kinematic slavery, i.e., points on the surface of the body remain on the surface at all times. In analogy to the volume, we formally introduce the surface gradient and surface divergence of any field $\{\circ\}(\hat{\mathbf{X}}, t)$ defined on the surface

$$\hat{\nabla}\{\circ\} = \nabla\{\circ\} \cdot \hat{\mathbf{I}} \quad \text{and} \quad \widehat{\text{Div}}\{\circ\} = \nabla\{\circ\} : \hat{\mathbf{I}}, \quad (9)$$

where $\hat{\mathbf{I}} = \mathbf{I} - \mathbf{N} \otimes \mathbf{N}$ is the second order surface unit tensor, which serves as surface projection operator. With the above definitions, we introduce the surface deformation gradient $\hat{\mathbf{F}} : S_0 \rightarrow S_t$, which maps tangential line elements to the material surface $d\hat{\mathbf{X}} \in S_0$ onto tangential line elements to the spatial surface $d\hat{\mathbf{x}} \in S_t$. Similar to the volume deformation gradient \mathbf{F} , the surface deformation gradient $\hat{\mathbf{F}}$ obeys a multiplicative decomposition into an elastic part $\hat{\mathbf{F}}^e$ and a growth part $\hat{\mathbf{F}}^g$

$$\hat{\mathbf{F}} = \hat{\nabla} \hat{\phi} = \mathbf{F} \cdot \hat{\mathbf{I}} \quad \text{with} \quad \hat{\mathbf{F}} = \hat{\mathbf{F}}^e \cdot \hat{\mathbf{F}}^g. \quad (10)$$

In contrast to the surface deformation gradient $\hat{\mathbf{F}}$, however, neither $\hat{\mathbf{F}}^e$ nor $\hat{\mathbf{F}}^g$ are necessarily restricted to result from the projection of the corresponding volume quantities \mathbf{F}^e and \mathbf{F}^g . Although the surface deformation gradient and its elastic and growth part are noninvertible, they possess inverses in the generalized sense, $\hat{\mathbf{f}} \cdot \hat{\mathbf{F}} = \hat{\mathbf{I}}$, $\hat{\mathbf{f}}^e \cdot \hat{\mathbf{F}}^e = \hat{\mathbf{I}}$, and $\hat{\mathbf{f}}^g \cdot \hat{\mathbf{F}}^g = \hat{\mathbf{I}}$ in terms of the surface unit tensor $\hat{\mathbf{I}}$. In analogy to the volume Jacobian J , we can introduce the Jacobian \hat{J} of the surface deformation gradient $\hat{\mathbf{F}}$, which relates material surface area elements $dA_0 \in S_0$ and spatial surface area elements $dA_t \in S_t$ as $dA_t = \hat{J} dA_0$. Similarly, we decompose the surface Jacobian multiplicatively into an elastic part \hat{J}^e and a growth part \hat{J}^g

$$\hat{J} = \widehat{\det}(\hat{\mathbf{F}}) = \|\text{cof}(\mathbf{F}) \cdot \mathbf{N}\| > 0 \quad \text{with} \quad \hat{J} = \hat{J}^e \hat{J}^g. \quad (11)$$

Here $\text{cof}(\circ) = \det(\circ)(\circ)^{-t}$ denotes the cofactor of the second order tensor (\circ) . We can then express the elastic surface Jacobian as $\hat{J}^e = \hat{J}/\hat{J}^g$ and the growth surface Jacobian as $\hat{J}^g = \widehat{\det}(\hat{\mathbf{F}}^g)$ in terms of the covariant base vectors \mathbf{A}_α in TS_0 (Gurtin and Struthers, 1990)

$$\widehat{\det}(\hat{\mathbf{F}}^g) = \frac{|[\hat{\mathbf{F}}^g \cdot \mathbf{A}_1] \times [\hat{\mathbf{F}}^g \cdot \mathbf{A}_2]|}{|\mathbf{A}_1 \times \mathbf{A}_2|}. \quad (12)$$

Finally, we introduce the right Cauchy Green surface tensor $\hat{\mathbf{C}}$ in the material configuration and its elastic counterpart $\hat{\mathbf{C}}^e$ in the intermediate configuration as characteristic surface deformation measures

$$\hat{\mathbf{C}} = \hat{\mathbf{F}}^t \cdot \hat{\mathbf{F}} \quad \text{and} \quad \hat{\mathbf{C}}^e = \hat{\mathbf{F}}^{et} \cdot \hat{\mathbf{F}}^e, \quad (13)$$

which are related through the identity, $\hat{\mathbf{C}}^e = \hat{\mathbf{f}}^{g,t} \cdot \hat{\mathbf{C}} \cdot \hat{\mathbf{f}}^g$. In analogy to the volume considerations, we introduce the pull back of the spatial surface velocity gradient $\hat{\mathbf{I}}$ to the intermediate configuration

$$\hat{\mathbf{I}} = \mathbf{D}_t \hat{\mathbf{F}} \cdot \hat{\mathbf{f}} \quad \text{with} \quad \hat{\mathbf{f}}^e \cdot \hat{\mathbf{I}} \cdot \hat{\mathbf{F}}^e = \hat{\mathbf{L}}^e + \hat{\mathbf{L}}^g, \quad (14)$$

which obeys an additive decomposition into the elastic surface velocity gradient $\hat{\mathbf{L}}^e = \hat{\mathbf{f}}^e \cdot \mathbf{D}_t \hat{\mathbf{F}}^e$ and the growth surface velocity gradient $\hat{\mathbf{L}}^g = \mathbf{D}_t \hat{\mathbf{F}}^g \cdot \hat{\mathbf{f}}^g$.

Remark 1. The material and spatial second order surface unit tensors $\hat{\mathbf{I}} = \mathbf{I} - \mathbf{N} \otimes \mathbf{N}$ and $\hat{\mathbf{i}} = \mathbf{I} - \mathbf{n} \otimes \mathbf{n}$ serve as projection tensors to map the volume deformation gradient and its inverse onto their surface counterparts

$$\begin{aligned} \hat{\mathbf{F}} &= \mathbf{F} \cdot \hat{\mathbf{I}}, \quad \text{with} \quad \hat{\mathbf{I}} = \mathbf{I} - \mathbf{N} \otimes \mathbf{N}, \\ \hat{\mathbf{f}} &= \mathbf{f} \cdot \hat{\mathbf{i}}, \quad \text{with} \quad \hat{\mathbf{i}} = \mathbf{I} - \mathbf{n} \otimes \mathbf{n}, \end{aligned} \quad (15)$$

where \mathbf{N} and $\mathbf{n} = \mathbf{N} \cdot \mathbf{f} / |\mathbf{N} \cdot \mathbf{f}|$ are the unit outward normals to the material and spatial surfaces. Since the surface unit tensors $\hat{\mathbf{I}}$ and $\hat{\mathbf{i}}$ are rank deficient, the surface deformation gradient is noninvertible. However, it possesses a generalized

inverse according to the following singular value decomposition:

$$\begin{aligned}\hat{\mathbf{f}} \cdot \hat{\mathbf{F}} &= \hat{\mathbf{I}}, & \hat{\mathbf{F}} &= \mathbf{U} \cdot \boldsymbol{\Sigma} \cdot \mathbf{V}^t, & \hat{\mathbf{f}} &= \mathbf{V} \cdot [\boldsymbol{\Sigma}^+]^{-1} \cdot \mathbf{U}^t \\ \hat{\mathbf{f}}^t \cdot \hat{\mathbf{F}}^t &= \hat{\mathbf{I}}, & \hat{\mathbf{F}}^t &= \mathbf{U} \cdot \boldsymbol{\sigma} \cdot \mathbf{V}^t, & \hat{\mathbf{f}}^t &= \mathbf{V} \cdot [\boldsymbol{\sigma}^+]^{-1} \cdot \mathbf{U}^t,\end{aligned}\quad (16)$$

where the diagonal entries of $\boldsymbol{\Sigma}$ and $\boldsymbol{\sigma}$ correspond to the singular values of $\hat{\mathbf{F}}$ and $\hat{\mathbf{F}}^t$, the columns of \mathbf{U} and \mathbf{V} are the left- and right-singular vectors associated with these singular values, and $\boldsymbol{\Sigma}^+$ and $\boldsymbol{\sigma}^+$ are the pseudoinverses of $\boldsymbol{\Sigma}$ and $\boldsymbol{\sigma}$, which are formed by replacing every nonzero diagonal entry by its reciprocal value.

3. Balance equations of growth

3.1. Balance equations of volume growth

The balance of mass for growing continua balances the rate of change of the material volume density ρ_0 with the volume mass source \mathcal{R}_0 and the volume mass flux \mathbf{R} (Kuhl and Steinmann, 2003a, 2003b). For simplicity, we assume the mass flux to be negligibly small, $\mathbf{R} = \mathbf{0}$, such that

$$D_t \rho_0 = \mathcal{R}_0 \quad \text{or} \quad \rho_0(t) = \rho_0(t_0) + \int_{t_0}^t \mathcal{R}_0(\tau) \, d\tau. \quad (17)$$

By using the volume Jacobians introduced in Eq. (4), we immediately obtain the following relations between the volume densities in the material, spatial, and intermediate configurations ρ_0 , ρ_t , and ρ_g

$$\rho_0 = J \rho_t = J^g \rho_g \quad \text{such that} \quad D_t \rho_0 = J^g D_t \mathbf{F}^g : \mathbf{f}^g \rho_g + J^g D_t \rho_g = J^g [\rho_g \operatorname{tr} \mathbf{L}^g + D_t \rho_g]. \quad (18)$$

In the transformation above, we have utilized the time derivative of J^g as $D_t J^g = \partial_{\mathbf{F}^g} J^g : D_t \mathbf{F}^g = J^g [\mathbf{f}^g]^t : D_t \mathbf{F}^g = J^g \operatorname{tr} \mathbf{L}^g$. The combination of Eqs. (17.1) and (18.2) renders the following explicit representation of the mass source \mathcal{R}_0

$$\mathcal{R}_0 = J^g [\rho_g \operatorname{tr} \mathbf{L}^g + D_t \rho_g]. \quad (19)$$

The balance of linear momentum balances the rate of change of the linear momentum, which we assume to vanish here for the quasi-static case, with the divergence of the volume Piola stresses \mathbf{P} and the volume forces \mathbf{b}

$$\mathbf{0} = \operatorname{Div} \mathbf{P} + \mathbf{b}. \quad (20)$$

The Piola stresses \mathbf{P} and volume forces \mathbf{b} have the dimensions force per unit area and force per unit volume. We obtain the weak form of the balance of linear momentum (20) through the standard multiplication with the test function $\delta \boldsymbol{\varphi}$, integration over the volume B_0 , and integration by parts

$$\int_{B_0} \nabla \delta \boldsymbol{\varphi} : \mathbf{P} \, dV_0 = \int_{B_0} \delta \boldsymbol{\varphi} \cdot \mathbf{b} \, dV_0 + \int_{S_0} \delta \boldsymbol{\varphi} \cdot \mathbf{P} \cdot \mathbf{N} \, dA_0. \quad (21)$$

Here, the lefthand side characterizes the internal forces, and the righthand side terms represent the external volume forces and the external surface forces. Alternatively, we could rephrase the weak form in terms of the Piola Kirchhoff stress \mathbf{S} or the Cauchy stress $\boldsymbol{\sigma}$

$$\mathbf{S} = \mathbf{f} \cdot \mathbf{P}, \quad \text{and} \quad \boldsymbol{\sigma} = j \mathbf{P} \cdot \mathbf{F}^t, \quad (22)$$

such that the internal force term of the weak form (21) takes the following alternative representations:

$$\int_{B_0} \nabla \delta \boldsymbol{\varphi} : \mathbf{P} \, dV_0 = \int_{B_0} [\mathbf{F}^t \cdot \nabla \delta \boldsymbol{\varphi}] : \mathbf{S} \, dV_0 = \int_{B_t} [\nabla \delta \boldsymbol{\varphi} : \mathbf{f}] : \boldsymbol{\sigma} \, dV_t. \quad (23)$$

3.2. Balance equations of surface growth

The balance of mass for growing surfaces balances the rate of change of the material area density $\hat{\rho}_0$ with the area mass source $\hat{\mathcal{R}}_0$ and the area mass flux $\hat{\mathbf{R}}$, which we again assume to vanish in the sequel, $\hat{\mathbf{R}} = \mathbf{0}$, such that

$$D_t \hat{\rho}_0 = \hat{\mathcal{R}}_0 \quad \text{or} \quad \hat{\rho}_0(t) = \hat{\rho}_0(t_0) + \int_{t_0}^t \hat{\mathcal{R}}_0(\tau) \, d\tau. \quad (24)$$

We can then relate the surface densities in the material, spatial, and intermediate configurations $\hat{\rho}_0$, $\hat{\rho}_t$, and $\hat{\rho}_g$ with the help of the surface Jacobians (11)

$$\hat{\rho}_0 = \hat{J} \hat{\rho}_t = \hat{J}^g \hat{\rho}_g \quad \text{such that} \quad D_t \hat{\rho}_0 = \hat{J}^g D_t \hat{\mathbf{F}}^g : \hat{\mathbf{f}}^g \hat{\rho}_g + \hat{J}^g D_t \hat{\rho}_g = \hat{J}^g [\hat{\rho}_g \hat{\mathbf{L}}^g + D_t \hat{\rho}_g], \quad (25)$$

where $D_t \hat{J}^g = \partial_{\hat{\mathbf{F}}^g} \hat{J}^g : D_t \hat{\mathbf{F}}^g = \hat{J}^g [\hat{\mathbf{f}}^g]^t : D_t \hat{\mathbf{F}}^g = \hat{J}^g \operatorname{tr} \hat{\mathbf{L}}^g$. The mass source then follows directly from the combination of Eqs. (24.1) and (25.2) as

$$\hat{\mathcal{R}}_0 = \hat{J}^g [\hat{\rho}_g \operatorname{tr} \hat{\mathbf{L}}^g + D_t \hat{\rho}_g]. \quad (26)$$

The balance of linear momentum balances the rate of change of the linear surface momentum, which we assume to be negligible in the quasi-static case, with the divergence of the surface stresses $\hat{\mathbf{P}}$ and the surface tractions $\hat{\mathbf{b}} - \mathbf{P} \cdot \mathbf{N}$

$$\mathbf{0} = \widehat{\text{Div}} \hat{\mathbf{P}} + [\hat{\mathbf{b}} - \mathbf{P} \cdot \mathbf{N}]. \quad (27)$$

Here, the surface stresses $\hat{\mathbf{P}}$ and the surface tractions $\hat{\mathbf{b}} - \mathbf{P} \cdot \mathbf{N}$ have the dimensions force per unit length and force per unit area. The surface tractions consist of two contributions, the prescribed surface tractions $\hat{\mathbf{b}}$ and the surface tractions imposed by the underlying volume through the projected volume Piola stress $\mathbf{P} \cdot \mathbf{N}$ (Steinmann, 2008). To transform the balance of linear surface momentum into its weak form, we multiply it with the test function $\delta\varphi$, integrate it over the surface S_0 , and apply the integration by parts

$$\int_{S_0} \widehat{\nabla} \delta\varphi : \hat{\mathbf{P}} \, dA_0 = \int_{S_0} \delta\varphi \cdot \hat{\mathbf{b}} \, dA_0 - \int_{S_0} \delta\varphi \cdot \mathbf{P} \cdot \mathbf{N} \, dA_0 + \int_{C_0} \delta\varphi \cdot \hat{\mathbf{P}} \cdot \mathbf{N} \, dL_0. \quad (28)$$

The lefthand side characterizes the internal surface forces, and the righthand side terms represent the prescribed external surface forces, the projected external surface forces imposed by the underlying volume, and the external line forces along the boundary curve to the surface C_0 . Again, we can introduce the surface Piola Kirchhoff stress $\hat{\mathbf{S}}$ and the surface Cauchy stress $\hat{\boldsymbol{\sigma}}$ using the surface Piola transforms

$$\hat{\mathbf{S}} = \hat{\mathbf{f}} \cdot \hat{\mathbf{P}}, \text{ and } \hat{\boldsymbol{\sigma}} = \hat{\mathbf{j}} \hat{\mathbf{P}} \cdot \hat{\mathbf{F}}^t, \quad (29)$$

to rephrase the internal forces of the weak form (28) through the following expressions:

$$\int_{S_0} \widehat{\nabla} \delta\varphi : \hat{\mathbf{P}} \, dA_0 = \int_{S_0} [\hat{\mathbf{F}}^t \cdot \widehat{\nabla} \delta\varphi] : \hat{\mathbf{S}} \, dA_0 = \int_{S_t} [\widehat{\nabla} \delta\varphi \cdot \hat{\mathbf{f}}] : \hat{\boldsymbol{\sigma}} \, dA_t. \quad (30)$$

4. Constitutive equations

4.1. Constitutive equations of volume growth

To characterize volume growth in a hyperelastic medium, we introduce a Helmholtz free volume energy ψ , parameterized in terms of the elastic contribution to the volume deformation gradient \mathbf{F}^e , or, alternatively, in terms of the volume deformation gradient \mathbf{F} and the volume growth tensor \mathbf{F}^g

$$\psi = \psi(\mathbf{F}, \mathbf{F}^g) = \psi(\mathbf{F}^e). \quad (31)$$

The corresponding volume Piola stress \mathbf{P} follows from thermodynamic considerations as stress measure conjugate to the deformation gradient \mathbf{F}

$$\mathbf{P} = \frac{\partial \psi}{\partial \mathbf{F}} = \frac{\partial \psi}{\partial \mathbf{F}^e} : \frac{\partial \mathbf{F}^e}{\partial \mathbf{F}} = \mathbf{P}^e \cdot [\mathbf{f}^g]^t \text{ with } \mathbf{P}^e = \frac{\partial \psi}{\partial \mathbf{F}^e}, \quad (32)$$

where \mathbf{P}^e denotes the classic elastic volume Piola stress. The total derivative of the Piola stress \mathbf{P} with respect to the deformation gradient \mathbf{F} introduces the fourth order tensor of tangent volume moduli \mathbb{A}

$$\mathbb{A} = \frac{d\mathbf{P}}{d\mathbf{F}} = \frac{d\mathbf{P}}{d\mathbf{F}^e} : \frac{d\mathbf{F}^e}{d\mathbf{F}} = \mathbb{A}^e : [[\mathbf{f}^g]^t \otimes [\mathbf{f}^g]^t] \text{ with } \mathbb{A}^e = \frac{d\mathbf{P}^e}{d\mathbf{F}^e}, \quad (33)$$

where \mathbb{A}^e denotes the classic elastic volume tangent moduli. To characterize the growth process, we need to specify a functional form for the volume growth tensor \mathbf{F}^g and its evolution in time. For the simplest case of isotropic volume growth, the volume growth tensor \mathbf{F}^g takes the following functional form, parameterized in terms of a single scalar-valued growth multiplier ϑ

$$\mathbf{F}^g = \vartheta \mathbf{I}, \quad (34)$$

such that $\vartheta = 1$ in the initial ungrown state, $\vartheta > 1$ characterizes volume growth, and $\vartheta < 1$ characterizes volume shrinkage. We propose the following simple exponential evolution equation for the growth multiplier, which we can integrate explicitly in time

$$D_t \vartheta = [\vartheta^{\max} - \vartheta_0] \exp(-t/\tau) / \tau \quad \text{thus } \vartheta = \vartheta_0 + [\vartheta^{\max} - \vartheta_0] [1 - \exp(-t/\tau)]. \quad (35)$$

Here, τ characterizes the velocity of volume growth, $\vartheta_0 = 1.0$ is the initial growth value, and ϑ^{\max} limits the maximum amount of growth toward which the growth multiplier ϑ converges with progressing time $t \rightarrow \infty$. Fig. 3 illustrates the temporal evolution of the growth multiplier ϑ , with an initial value $\vartheta_0 = 1.0$, for varying growth velocities τ at fixed $\vartheta^{\max} = 4.0$, left, and varying maximum growth ϑ^{\max} at fixed $\tau = 10$, right.

Remark 2 (Isotropic volume growth). The special case of isotropic volume growth, $\mathbf{F}^g = \vartheta \mathbf{I}$, has three immediate consequences. First, the volume growth tensor \mathbf{F}^g can be inverted explicitly, and the volume deformation gradient \mathbf{F} ,

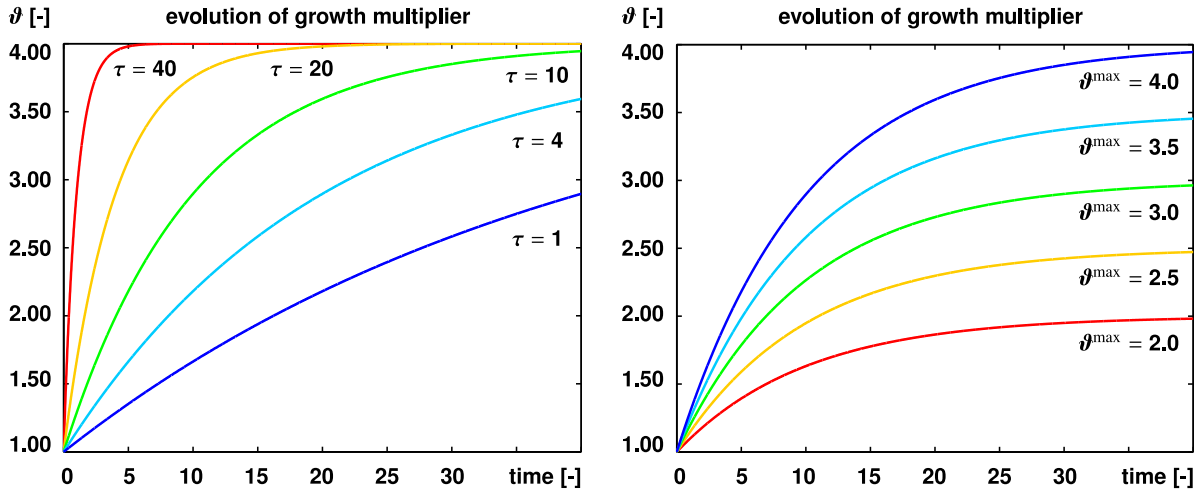


Fig. 3. Temporal evolution of growth multiplier ϑ for varying growth velocities τ at fixed ϑ^{\max} , left, and varying maximum growth ϑ^{\max} at fixed τ , right.

the volume Piola stress \mathbf{P} , and the volume tangent moduli \mathbb{A} become equal to their growth-weighted elastic counterparts

$$\mathbf{f}^g = \frac{1}{\vartheta} \mathbf{I} \quad \text{such that} \quad \mathbf{F} = \vartheta \mathbf{F}^e \quad \text{and} \quad \mathbf{P} = \frac{1}{\vartheta} \mathbf{P}^e \quad \text{and} \quad \mathbb{A} = \frac{1}{\vartheta^2} \mathbb{A}^e. \quad (36)$$

Second, the growth tensor \mathbf{F}^g always remains isotropic, and so does the volume growth velocity gradient \mathbf{L}^g

$$\mathbf{D}_t \mathbf{F}^g = \mathbf{D}_t \vartheta \mathbf{I} \quad \text{such that} \quad \mathbf{L}^g = \frac{\mathbf{D}_t \vartheta}{\vartheta} \mathbf{I}. \quad (37)$$

Third, volume changes upon growth J^g are simply equivalent to the third power of the growth multiplier ϑ

$$J^g = \vartheta^3 \quad \text{such that} \quad \rho_0 = \vartheta^3 \rho_g. \quad (38)$$

Overall, the assumption of isotropic growth significantly simplifies the general equations of volumetric growth.

Remark 3 (Growth at constant volume density). A common additional assumption is that the newly grown material has the same volume density as the original substrate (Menzel and Kuhl, 2012), $\mathbf{D}_t \rho_g = 0$. This implies that the volume density source \mathcal{R}_0 required to maintain a constant volume density in the intermediate configuration takes the following form:

$$\rho_g = \text{const.} \quad \text{such that} \quad \mathcal{R}_0 = \rho_0 \text{tr} \mathbf{L}^g = J^g \rho_g \mathbf{D}_t \mathbf{F}^g \cdot \mathbf{f}^g = 3 \rho_g \vartheta \mathbf{D}_t \vartheta. \quad (39)$$

For this special case, we do not need to discretize the balance of mass (17) explicitly, but can simply evaluate overall mass changes in a straightforward post-processing step.

4.2. Constitutive equations of surface growth

To characterize surface growth, we equip the surface with its own Helmholtz free surface energy $\hat{\psi}$, which we parameterize in terms of the elastic contribution to the surface deformation gradient $\hat{\mathbf{F}}^e$, or, alternatively, in terms of the surface deformation gradient $\hat{\mathbf{F}}$ and the surface growth tensor $\hat{\mathbf{F}}^g$

$$\hat{\psi} = \hat{\psi}(\hat{\mathbf{F}}, \hat{\mathbf{F}}^g) = \hat{\psi}(\hat{\mathbf{F}}^e). \quad (40)$$

For simplicity, we assume the surface to behave isotropically (Steinmann, 2008), and do not account for an explicit dependence on the deformed surface plane normal \mathbf{n} . Similar to the volume, we introduce the surface Piola stress $\hat{\mathbf{P}}$ as thermodynamically conjugate to the surface deformation gradient $\hat{\mathbf{F}}$

$$\hat{\mathbf{P}} = \frac{\partial \hat{\psi}}{\partial \hat{\mathbf{F}}} = \frac{\partial \hat{\psi}}{\partial \hat{\mathbf{F}}^e} : \frac{\partial \hat{\mathbf{F}}^e}{\partial \hat{\mathbf{F}}} = \hat{\mathbf{P}}^e \cdot [\hat{\mathbf{F}}^g]^t \quad \text{with} \quad \hat{\mathbf{P}}^e = \frac{\partial \hat{\psi}}{\partial \hat{\mathbf{F}}^e}, \quad (41)$$

where $\hat{\mathbf{P}}^e$ denotes the elastic surface Piola stress. Additionally, we introduce the fourth order tensor of tangent surface moduli $\hat{\mathbb{A}}$ as the total derivative of the Piola stress $\hat{\mathbf{P}}$ with respect to the deformation gradient $\hat{\mathbf{F}}$

$$\hat{\mathbb{A}} = \frac{d\hat{\mathbf{P}}}{d\hat{\mathbf{F}}} = \frac{d\hat{\mathbf{P}}}{d\hat{\mathbf{F}}^e} : \frac{d\hat{\mathbf{F}}^e}{d\hat{\mathbf{F}}} = \hat{\mathbb{A}}^e : [\hat{\mathbf{F}}^g]^t \otimes [\hat{\mathbf{F}}^g]^t \quad \text{with} \quad \hat{\mathbb{A}}^e = \frac{d\hat{\mathbf{P}}^e}{d\hat{\mathbf{F}}^e}, \quad (42)$$

such that $\hat{\mathbb{A}}^e$ denotes the elastic surface tangent moduli. Again, we consider the simplest possible case of growth, isotropic surface growth, for which the surface growth tensor $\hat{\mathbf{F}}^g$ can be parameterized in terms of a single scalar-valued growth

multiplier $\hat{\vartheta}$

$$\hat{\mathbf{F}}^g = \hat{\vartheta} \hat{\mathbf{I}}. \quad (43)$$

Similar to the case of volume growth, $\hat{\vartheta} = 1$ characterizes the initial ungrown state, $\hat{\vartheta} > 1$ corresponds to surface growth, and $\hat{\vartheta} < 1$ to surface shrinkage. Again, we suggest a simple exponential evolution equation for the growth multiplier, and integrate it explicitly in time

$$D_t \hat{\vartheta} = [\hat{\vartheta}^{\max} - \hat{\vartheta}_0] \exp(-t/\hat{\tau}) / \hat{\tau} \text{ thus } \hat{\vartheta} = \hat{\vartheta}_0 + [\hat{\vartheta}^{\max} - \hat{\vartheta}_0][1 - \exp(-t/\hat{\tau})]. \quad (44)$$

Here, $\hat{\tau}$ characterizes the velocity of surface growth, $\hat{\vartheta}_0 = 1.0$ is the initial growth value, and $\hat{\vartheta}^{\max}$ limits the maximum amount of surface growth toward which the growth multiplier $\hat{\vartheta}$ converges with progressing time t . Fig. 3 illustrates the temporal evolution of the growth multiplier $\hat{\vartheta}$, with an initial value $\hat{\vartheta}_0 = 1.0$, for varying growth velocities $\hat{\tau}$ at fixed $\hat{\vartheta}^{\max} = 4.0$, left, and varying maximum growth $\hat{\vartheta}^{\max}$ at fixed $\hat{\tau} = 10$, right.

Remark 4 (Isotropic surface growth). The special case of isotropic surface growth, $\hat{\mathbf{F}}^g = \hat{\vartheta} \hat{\mathbf{I}}$, has three immediate consequences. First, we can explicitly invert the surface growth tensor $\hat{\mathbf{F}}^g$ using the surface unit tensor $\hat{\mathbf{I}}$. This allows us to express the surface deformation gradient \mathbf{F} , the surface Piola stress \mathbf{P} , and the surface tangent moduli \mathbb{A} through to their growth-weighted elastic counterparts,

$$\hat{\mathbf{f}}^g = \frac{1}{\hat{\vartheta}} \hat{\mathbf{I}} \text{ such that } \hat{\mathbf{F}} = \hat{\vartheta} \hat{\mathbf{F}}^e \text{ and } \hat{\mathbf{P}} = \frac{1}{\hat{\vartheta}} \hat{\mathbf{P}}^e \text{ and } \hat{\mathbb{A}} = \frac{1}{\hat{\vartheta}^2} \hat{\mathbb{A}}^e. \quad (45)$$

Second, the surface growth tensor \mathbf{F}^g and the surface growth velocity gradient \mathbf{L}^g always remain isotropic

$$D_t \hat{\mathbf{F}}^g = D_t \hat{\vartheta} \hat{\mathbf{I}} \text{ such that } \hat{\mathbf{L}}^g = \frac{D_t \hat{\vartheta}}{\hat{\vartheta}} \hat{\mathbf{I}}. \quad (46)$$

Third, surface area changes upon growth $\hat{\mathbf{f}}^g$ are simply equivalent to the growth multiplier $\hat{\vartheta}$ squared

$$\hat{\mathbf{j}}^g = \hat{\vartheta}^2 \text{ such that } \hat{\rho}_0 = \hat{\vartheta}^2 \hat{\rho}_g. \quad (47)$$

As the above considerations indicate, the assumption of isotropic growth simplifies the governing equations of surface growth.

Remark 5 (Growth at constant surface density). If we additionally assume that the newly grown surface has the same surface density as the original surface, $D_t \hat{\rho}_g = 0$, we can express the surface density source $\hat{\mathcal{R}}_0$ in the following form:

$$\hat{\rho}_g = \text{const.} \text{ such that } \hat{\mathcal{R}}_0 = \hat{\rho}_0 \text{tr} \hat{\mathbf{L}}^g = \hat{\mathbf{j}}^g \hat{\rho}_g D_t \hat{\mathbf{F}}^g : \hat{\mathbf{f}}^g = 2 \hat{\rho}_g \hat{\vartheta} D_t \hat{\vartheta}. \quad (48)$$

Similar to the case of constant volume density, we do not need to discretize the balance of mass (24) explicitly, but can simply evaluate overall mass changes in a straightforward post-processing step.

5. Discretization

The governing equations for finite volume and surface growth are complex and highly nonlinear. In this section, we illustrate their computational solution within an incremental iterative nonlinear finite element framework. To characterize the state of the growth process at each instant in time, we introduce the volume and surface growth multipliers ϑ^g and $\hat{\vartheta}^g$ as internal variables, and solve their evolution Eqs. (35) and (44) locally at the integration point level. We begin by summarizing the residual of the weak forms of the balance of linear momentum in the volume (21) and on the surface (28)

$$\int_{B_0} \nabla \delta \boldsymbol{\varphi} : \mathbf{P} \, dV_0 - \int_{B_0} \delta \boldsymbol{\varphi} \cdot \mathbf{b} \, dV_0 + \int_{S_0} \hat{\nabla} \delta \boldsymbol{\varphi} : \hat{\mathbf{P}} \, dA_0 - \int_{S_0} \delta \boldsymbol{\varphi} \cdot \hat{\mathbf{b}} \, dA_0 - \int_{C_0} \delta \boldsymbol{\varphi} \cdot \hat{\mathbf{P}} \cdot \mathbf{N} \, dL_0 \doteq 0. \quad (49)$$

To discretize the weak form (49) in space, we partition the domain of interest $B_0 = \mathbf{U}_{e=1}^{n_{be}} B_0^e$ into n_{be} finite volume elements B_0^e , and the surface of interest $S_0 = \mathbf{U}_{e=1}^{n_{se}} S_0^e$ into n_{se} finite surface elements S_0^e . Although it is in principle possible to select arbitrary surface elements with independent nodes, it proves efficient to discretize the surface in consistency with the bulk. This implies that each surface element shares its nodes with its corresponding volume elements as illustrated in Fig. 4. The surface element itself then acts like a shell element, which moves in consistency with the bulk; however, it is equipped with its own independent free energy function. In the following subsections, we demonstrate the finite element discretizations of the volume and surface terms of Eq. (49), to obtain the discrete residual

$$\mathbf{R}_I = \mathbf{A} \int_{e=1}^{n_{el}} \nabla N^i \cdot \mathbf{P} \, dV_e - \int_{B_0^e} N^i \mathbf{b} \, dV_e + \int_{S_0^e} \hat{\nabla} N^i \cdot \hat{\mathbf{P}} \, dA_e - \int_{S_0^e} \hat{N}^i \hat{\mathbf{b}} \, dA_e - \int_{C_0^e} \hat{N}^i \hat{\mathbf{P}} \cdot \mathbf{N} \, dL_e \doteq 0. \quad (50)$$

Herein, the operator \mathbf{A} symbolizes the assembly of all element residuals at the $i = 1, \dots, n_{vn}$ volume element nodes to the global residual at the global node points $I = 1, \dots, n_{gn}$. To solve the above equation, we suggest an incremental iterative Newton algorithm based on the consistent linearization of the residual \mathbf{R}_I with respect to the nodal vector of unknowns $\boldsymbol{\varphi}_I$.

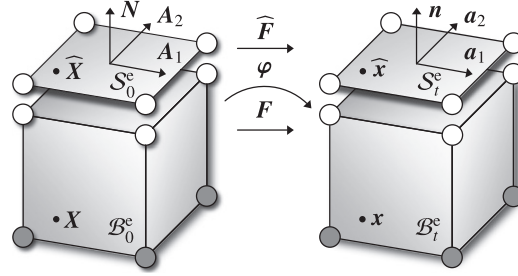


Fig. 4. Discretization of material body with finite volume elements \mathcal{B}_0^e and \mathcal{B}_t^e and of its surface with finite surface elements \mathcal{S}_0^e and \mathcal{S}_t^e . Surface elements share their nodes with the corresponding volume elements, however, they are equipped with their own energies $\hat{\psi}$, stresses $\hat{\mathbf{P}} = \partial \hat{\psi} / \partial \hat{\mathbf{F}}$, and tangent operators $\hat{\mathbb{A}} = d\hat{\mathbf{P}}/d\hat{\mathbf{F}}$.

This linearization introduces the global stiffness matrix at all global nodes $I, J = 1, \dots, n_{ng}$

$$\mathbf{K}_{IJ} = \frac{d\mathbf{R}_I}{d\varphi_J} = \sum_{e=1}^{n_{el}} \int_{\mathcal{B}_0^e} [\mathbf{I} \cdot \nabla N^i] : \hat{\mathbb{A}} \cdot \nabla N^j dV_e + \int_{\mathcal{S}_0^e} [\hat{\mathbf{I}} \cdot \hat{\nabla} N^i] : \hat{\mathbb{A}} \cdot \hat{\nabla} N^j dA_e. \quad (51)$$

For each global Newton iteration step, we iteratively update the current deformation state $\varphi_J \leftarrow \varphi_J - \mathbf{K}_{IJ}^{-1} \cdot \mathbf{R}_I$ until we achieve algorithmic convergence. Upon convergence, we store the volume and surface growth multipliers \mathcal{G}^g and $\hat{\mathcal{G}}^g$ at the integration points of the corresponding volume and surface elements.

5.1. Discretization of volume terms

To approximate the test functions $\delta\varphi$, trial functions φ , and nodal coordinates \mathbf{X} in the volume, we apply an isoparametric Bubnov–Galerkin type finite element interpolation

$$\delta\varphi = \sum_{i=1}^{n_{vn}} N^i \delta\varphi_i \quad \text{and} \quad \varphi = \sum_{j=1}^{n_{vn}} N^j \varphi_j \quad \text{and} \quad \mathbf{X} = \sum_{i=1}^{n_{vn}} N^i \mathbf{X}_i, \quad (52)$$

where N^i and N^j are the element shape functions in the volume and $i, j = 1, \dots, n_{vn}$ are nodes of the volume element. The gradients of the test and trial functions $\delta\mathbf{F} = \nabla \delta\varphi$ and $\mathbf{F} = \nabla \varphi$ then follow naturally in terms of the gradients of the shape functions ∇N^i and ∇N^j

$$\delta\mathbf{F} = \nabla \delta\varphi = \sum_{i=1}^{n_{vn}} \delta\varphi_i \otimes \nabla N^i \quad \text{and} \quad \mathbf{F} = \nabla \varphi = \sum_{j=1}^{n_{vn}} \varphi_j \otimes \nabla N^j. \quad (53)$$

To determine the gradients of the shape functions ∇N^i , we use the isoparametric concept for the approximation of the nodal coordinates \mathbf{X} from (52.3) to calculate the Jacobi matrix \mathbf{J} and its transposed inverse \mathbf{J}^{-t}

$$\nabla N^i = \frac{dN^i(\xi)}{d\mathbf{X}} = \frac{dN^i(\xi)}{d\xi} \cdot \frac{d\xi}{d\mathbf{X}} = \mathbf{J}^{-t} \cdot \frac{dN^i(\xi)}{d\xi} \quad \text{with} \quad \mathbf{J} = \frac{d\mathbf{X}}{d\xi} \quad \text{from} \quad \mathbf{X} = \sum_{i=1}^{n_{vn}} N^i(\xi) \mathbf{X}_i. \quad (54)$$

5.2. Discretization of surface terms

To approximate the test functions $\delta\varphi$, trial functions φ , and nodal coordinates \mathbf{X} on the surface, we apply a Bubnov–Galerkin type finite element interpolation

$$\delta\varphi = \sum_{i=1}^{n_{sn}} \hat{N}^i \delta\varphi_i \quad \text{and} \quad \varphi = \sum_{j=1}^{n_{sn}} \hat{N}^j \varphi_j \quad \text{and} \quad \mathbf{X} = \sum_{i=1}^{n_{sn}} \hat{N}^i \mathbf{X}_i, \quad (55)$$

where \hat{N}^i and \hat{N}^j are the element shape functions on the surface and $i, j = 1, \dots, n_{sn}$ are nodes of the surface element. The gradients of the test and trial functions $\delta\mathbf{F} = \hat{\nabla} \delta\varphi$ and $\mathbf{F} = \hat{\nabla} \varphi$ on the surface follow in terms of the covariant spatial base vectors $\delta\mathbf{a}_\alpha$ and \mathbf{a}_α multiplied with the contravariant material base vectors \mathbf{A}^α , for $\alpha = 1, 2$, such that

$$\delta\mathbf{F} = \hat{\nabla} \delta\varphi = \delta\mathbf{a}_\alpha \otimes \mathbf{A}^\alpha \quad \text{and} \quad \mathbf{F} = \hat{\nabla} \varphi = \mathbf{a}_\alpha \otimes \mathbf{A}^\alpha. \quad (56)$$

Accordingly, we first calculate the covariant spatial and material base vectors $\delta\mathbf{a}_\alpha$, \mathbf{a}_α , and \mathbf{A}_α , see Fig. 4, with

$$\delta\mathbf{a}_\alpha = \delta\varphi_{,\xi\alpha} = \sum_{i=1}^{n_{sn}} \delta\varphi_i \hat{N}_{,\xi\alpha}^i \quad \text{and} \quad \mathbf{a}_\alpha = \varphi_{,\xi\alpha} = \sum_{i=1}^{n_{sn}} \varphi_i \hat{N}_{,\xi\alpha}^i \quad \text{and} \quad \mathbf{A}_\alpha = \mathbf{X}_{,\xi\alpha} = \sum_{i=1}^{n_{sn}} \mathbf{X}_i \hat{N}_{,\xi\alpha}^i. \quad (57)$$

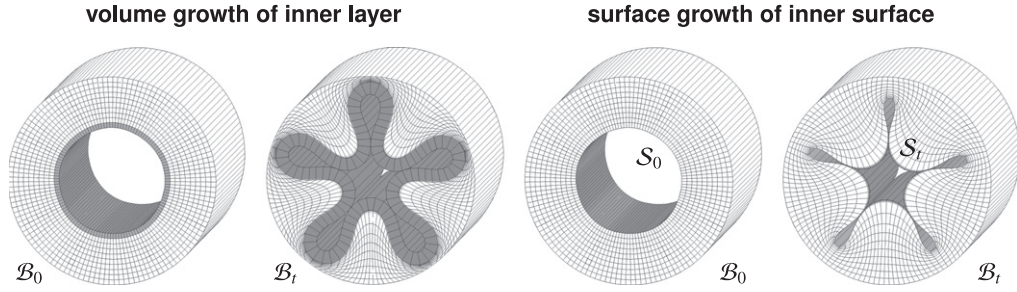


Fig. 5. Finite element discretization of cylindrical tube discretized with 10 elements in the radial, 125 elements in the circumferential, and one element in the longitudinal direction, resulting in a total of 1250 volume elements and 8250 degrees of freedom. To simulate volume growth, left, we allow the inner layer to grow, shown in gray, while the outer layer remains hyperelastic, shown in white. To simulate surface growth, right, we allow the inner surface to grow, shown in gray, while the entire bulk remains hyperelastic, shown in white.

Then, we determine the contravariant material base vectors \mathbf{A}^α using the contravariant and covariant material metric coefficients $A^{\alpha\beta}$ and $A_{\alpha\beta}$ for $\alpha, \beta = 1, 2$, such that

$$\mathbf{A}^\alpha = A^{\alpha\beta} \mathbf{A}_\beta \quad \text{with } A^{\alpha\beta} = \mathbf{A}^\alpha \cdot \mathbf{A}^\beta = [A_{\alpha\beta}]^{-1} \text{ and } A_{\alpha\beta} = \mathbf{A}_\alpha \cdot \mathbf{A}_\beta. \quad (58)$$

The gradients of the shape functions $\hat{\nabla} N^i$ follow in analogy to the volume, however, here, they are explicit functions of the contravariant base vectors \mathbf{A}^α

$$\hat{\nabla} N^i = \frac{d\hat{N}^i(\xi)}{d\mathbf{X}} = \frac{d\hat{N}^i(\xi)}{d\xi} \cdot \frac{d\xi}{d\mathbf{X}} = \hat{\mathbf{J}}^{-t} \cdot \frac{d\hat{N}^i(\xi)}{d\xi} \quad \text{with } \hat{\mathbf{J}} = \frac{d\mathbf{X}}{d\xi} = [\mathbf{A}_1, \mathbf{A}_2] \quad \text{and} \quad \hat{\mathbf{J}}^{-1} = \frac{d\xi}{d\mathbf{X}} = \begin{bmatrix} \mathbf{A}^1 \\ \mathbf{A}^2 \end{bmatrix}. \quad (59)$$

6. Results

To systematically compare the features of volume and surface growth, we simulate constrained growth of the inner lining of a cylindrical hyperelastic tube. The tube is 5 cm long, and has an initial inner and outer radius of 1 cm and 2 cm, see Fig. 5. Throughout the simulation, we apply homogeneous Dirichlet boundary conditions to the entire outer surface and to the axial deformation at the longitudinal boundaries. To initiate an inhomogeneous growth pattern, we perturb the inner surface with slight sinus-type perturbations of an amplitude of ± 0.005 cm.

6.1. Volume growth inside a cylindrical tube

To illustrate the features of volume growth, we allow a thin inner layer of a cylindrical tube to grow, while the thick outer layer remains entirely hyperelastic. We characterize the hyperelastic response of both layers through an isotropic Helmholtz volume energy ψ_0 of Neo–Hookean type

$$\psi_0 = \frac{1}{2} \mu [\mathbf{F}^e : \mathbf{F}^e - 3 - 2 \ln J^e] + \frac{1}{2} \lambda \ln^2 J^e,$$

where λ and μ are the standard volume Lamé constants. To evaluate the discrete residual (50) and its consistent linearization (51), we calculate the volume Piola stress \mathbf{P} using the general definition (32)

$$\mathbf{P} = \frac{\partial \psi_0}{\partial \mathbf{F}} = \frac{1}{J} \mathbf{P}^e \quad \text{with } \mathbf{P}^e = \frac{\partial \psi_0}{\partial \mathbf{F}^e} = \mu \mathbf{F}^e + [\lambda \ln J^e - \mu] [\mathbf{F}^e]^t,$$

and the volume tangent \mathbb{A} using the general definition (33)

$$\mathbb{A} = \frac{d\mathbf{P}}{d\mathbf{F}} = \frac{1}{J^2} \mathbb{A}^e \quad \text{with } \mathbb{A}^e = \frac{d\mathbf{P}^e}{d\mathbf{F}^e} = \mu \mathbf{I} \otimes \mathbf{I} + [\mu - \lambda \ln J^e] [\mathbf{F}^e]^t \otimes \mathbf{F}^e + \lambda [\mathbf{F}^e]^t \otimes [\mathbf{F}^e]^t,$$

along with the assumption of isotropic volume growth, $\mathbf{F}^s = J \mathbf{I}$, according to Eq. (34). Typically, the inner layer is considered significantly thinner and stiffer than the outer layer (Wiggs et al., 1997). For the thin growing inner layer, we choose a thickness of 0.1 cm, Lamé constants of $\lambda = 577$ N/mm² and $\mu = 385$ N/mm², a maximum growth of $g^{\max} = 4.0$, and a time constant of $\tau = 10.0$, see Fig. 3. For the thick elastic outer layer, the thickness is 0.9 cm, and we choose Lamé constants of $\lambda = 0.577$ N/mm² and $\mu = 0.385$ N/mm². We initiate an inhomogeneous growth pattern through a pentagonal perturbation of five sinus waves applied to the inner surface. We discretize the tube with 10 elements in the radial, 125 elements in the circumferential, and one element in the longitudinal direction, resulting in a total of 1250 volume elements and 8250 degrees of freedom. Fig. 5, left, shows the finite element discretization for volume growth, with the growing inner layer displayed in gray and the elastic outer layer displayed in white.

Table 1
Algorithmic performance. Quadratic convergence of the volume growth model.

ϑ	1.00	1.50	1.625	1.75	2.00
Step 1	1.0000E+00	1.0000E+00	1.0000E+00	1.0000E+00	1.0000E+00
Step 2	4.3747E-02	5.5751E-01	2.2976E-01	2.4441E-01	1.3236E-01
Step 3	7.2024E-04	3.7903E-02	2.7182E-04	7.9407E-04	4.5692E-04
Step 4	3.1095E-07	4.8239E-04	2.4654E-08	7.8617E-07	2.1001E-08
Step 5	3.4032E-13	3.6275E-08	4.9280E-14	6.0084E-13	6.9262E-12
Step 6	–	5.1057E-13	–	–	–
t	0.100	1.706	2.328	2.909	4.421
Δt	0.100	0.009	0.021	0.044	0.134

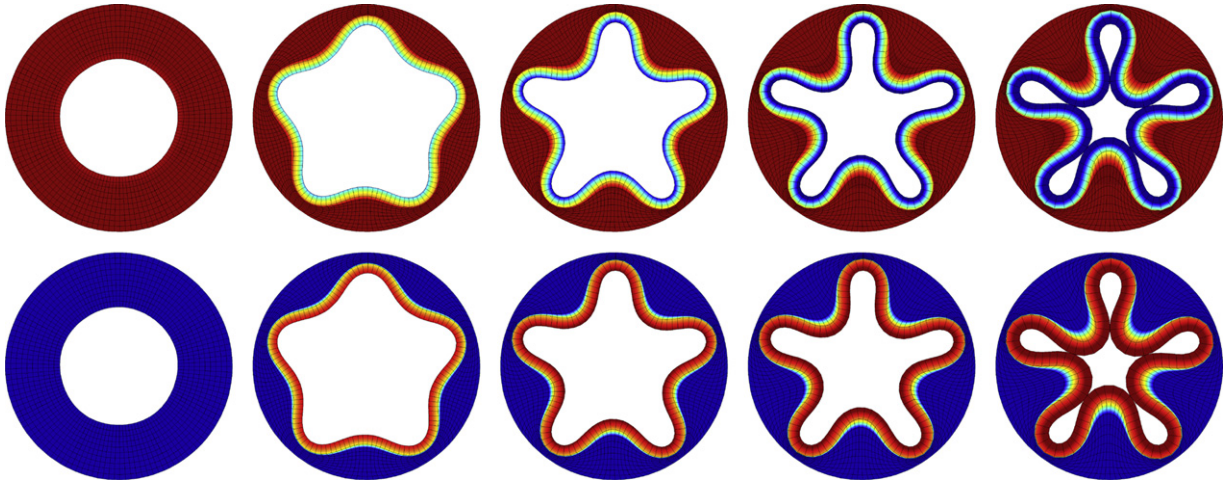


Fig. 6. Volume growth of inner layer of a cylindrical tube with pentagonally perturbed inner surface. Spatio-temporal evolution of radial stresses, top, and deviatoric stresses, bottom. The growing inner layer successively increases in volume, pulling the hyperelastic outer layer inward. As growth progresses, the pentagonal perturbation grows into five distinct inner folds. Snapshots correspond to $\vartheta = 1.00$, $\vartheta = 1.50$, $\vartheta = 1.625$, $\vartheta = 1.75$, and $\vartheta = 2.00$.

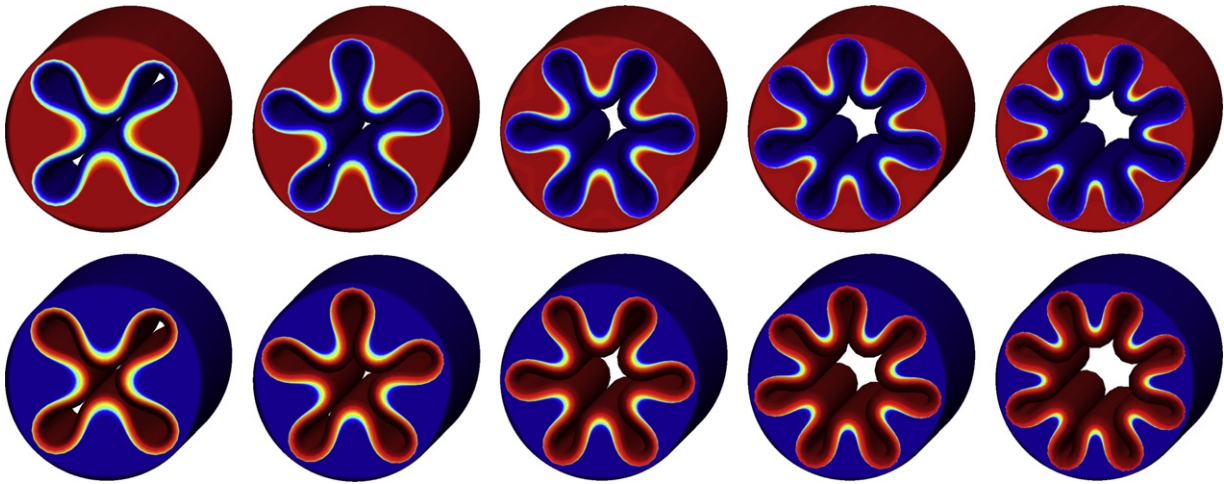


Fig. 7. Volume growth of inner layer of a cylindrical tube with perturbed inner surface. Spatial distribution of radial stresses, top, and deviatoric stresses, bottom. Square, pentagonal, hexagonal, heptagonal, and octagonal perturbations transition into four, five, six, seven, and eight distinct inner folds. Snapshots correspond to the time point of first self-contact, which occurs at $\vartheta = 1.87$ for square, at $\vartheta = 2.00$ for pentagonal, at $\vartheta = 2.19$ for hexagonal, at $\vartheta = 2.28$ for heptagonal, and at $\vartheta = 2.36$ for octagonal perturbations.

Table 1 demonstrates the algorithmic performance of the volume growth model. The five individual columns correspond to the snapshots displayed in Fig. 6. The algorithm converges quadratically in five to six iteration steps for a convergence criterion of $10E-10$. To accurately capture the growth process, we apply an ad hoc time adaptive scheme,

which automatically decreases the time step size by 50% once the number of Newton iterations exceeds seven, and increases the time step size by 10% otherwise. As the growth process progresses, the time step size decreases initially and then increases. The minimum time step size of $\Delta t^{\min} = 0.003$ at a volume growth multiplier of $\vartheta = 1.38$ corresponds exactly to the onset of buckling, when the five perturbations transition from an initially convex to an inward folded concave state.

Fig. 6 illustrates volume growth of the inner tubular layer at the discrete time points summarized in Table 1. The upper and lower rows display the spatio-temporal evolution of the radial and deviatoric stresses. As time progresses, the growing inner layer successively increases in volume, pulling the hyperelastic outer layer inward. During this growth process, the pentagonal perturbation grows into five distinct inner folds. Both radial and deviatoric stresses are concentrated in the growing inner layer, while the hyperelastic outer layer remains virtually stress free.

Fig. 7 provides a fully three-dimensional view of the volume growth process. To explore the impact of the degree of perturbation, we systematically vary the number of perturbations applied to the inner surface. Square, pentagonal, hexagonal, heptagonal, and octagonal perturbations, displayed from left to right, gradually transition into four, five, six, seven, and eight distinct inner folds. The upper and lower rows display the spatial distribution of the radial and deviatoric stresses. Both stress patterns are conceptually similar for different degrees of perturbation, displaying maximum stresses in the growing inner, while the hyperelastic outer layer remains virtually stress free. The illustrated snapshots correspond to the time point of first self-contact, which occurs at $\vartheta = 1.87$ for square, at $\vartheta = 2.00$ for pentagonal, at $\vartheta = 2.19$ for hexagonal, at $\vartheta = 2.28$ for heptagonal, and at $\vartheta = 2.36$ for octagonal perturbations.

6.2. Surface growth inside a cylindrical tube

To illustrate the features of surface growth, we allow the inner surface of a cylindrical tube to grow, while the entire bulk remains hyperelastic. We characterize the hyperelastic response of the inner surface through an isotropic Helmholtz surface energy ψ_0 of Neo Hookean type in analogy to its volumetric counterpart (Javili and Steinmann, 2010)

$$\hat{\psi}_0(\hat{\mathbf{F}}^e) = \frac{1}{2} \hat{\mu} [\hat{\mathbf{F}}^e : \hat{\mathbf{F}}^e - 2 - 2 \ln \hat{J}^e] + \frac{1}{2} \hat{\lambda} \ln^2 \hat{J}^e,$$

where $\hat{\lambda}$ and $\hat{\mu}$ are the surface Lamé constants. To evaluate the discrete residual (50) and its consistent linearization (51), we calculate the surface Piola stress $\hat{\mathbf{P}}$ using the general definition (41)

$$\hat{\mathbf{P}} = \frac{\partial \psi_0}{\partial \hat{\mathbf{F}}} = \frac{1}{\vartheta} \hat{\mathbf{P}}^e \quad \text{with} \quad \hat{\mathbf{P}}^e = \frac{\partial \psi_0}{\partial \hat{\mathbf{F}}^e} = \hat{\mu} \hat{\mathbf{F}}^e + [\hat{\lambda} \ln \hat{J}^e - \hat{\mu}] [\hat{\mathbf{f}}^e]^t,$$

and the surface tangent $\hat{\mathbb{A}}$ using the definition (42),

$$\hat{\mathbb{A}} = \frac{d\hat{\mathbf{P}}}{d\hat{\mathbf{F}}} = \frac{1}{\vartheta^2} \hat{\mathbb{A}}^e \quad \text{with} \quad \hat{\mathbb{A}}^e = \frac{d\hat{\mathbf{P}}^e}{d\hat{\mathbf{F}}^e} = \hat{\mu} \hat{\mathbf{I}} \otimes \hat{\mathbf{I}} + [\hat{\mu} - \hat{\lambda} \ln \hat{J}^e] [\hat{\mathbf{f}}^e]^t \otimes \hat{\mathbf{f}}^e - \hat{\mathbf{i}}^\perp \otimes [\hat{\mathbf{f}}^e \cdot [\hat{\mathbf{f}}^e]^t] + \hat{\lambda} [\hat{\mathbf{f}}^e]^t \otimes [\hat{\mathbf{f}}^e]^t,$$

along with the assumption of isotropic surface growth, $\hat{\mathbf{F}}^g = \hat{\vartheta} \hat{\mathbf{I}}$, according to Eq. (43). In the above equation, we have used the abbreviation $\hat{\mathbf{i}}^\perp$ for the second order normal projection tensor $\hat{\mathbf{i}}^\perp = \hat{\mathbf{i}} - \hat{\mathbf{i}} \otimes \hat{\mathbf{n}} = \mathbf{n} \otimes \mathbf{n}$. For the growing surface, we choose surface Lamé constants of $\hat{\lambda} = 0.577 \text{ N/mm}^2$ and $\hat{\mu} = 0.385 \text{ N/mm}^2$, a maximum growth of $\hat{\vartheta}^{\max} = 4.0$, and a time constant of $\hat{\tau} = 10.0$, see Fig. 3. For the elastic bulk, we choose volume Lamé constants of $\lambda = 0.577 \text{ N/mm}^2$ and $\mu = 0.385 \text{ N/mm}^2$. We initiate an inhomogeneous growth pattern through a pentagonal perturbation of five sinus waves applied to the inner growing surface. We discretize the tube with 10 elements in the radial, 125 elements in the circumferential, and one element in the longitudinal direction, resulting in a total of 1250 volume elements and 8250 degrees of freedom. In addition, we discretize the inner surface with 125 surface elements. Since these surface elements share their nodes with the corresponding volume elements, see Fig. 4, the addition of surface elements does not change the overall number of degrees of freedom. Fig. 5, right, shows the finite element discretization for surface growth, with the growing inner surface displayed in gray and the elastic bulk displayed in white.

Table 2 documents the algorithmic performance of the surface growth model. The five individual columns correspond to the snapshots displayed in Fig. 8. The algorithm converges quadratically in five iteration steps for a convergence criterion of $10\text{E}-10$. To accurately capture the growth process, we apply an ad hoc time adaptive scheme, which automatically decreases the time step size by 50% once the number of Newton iterations exceeds seven, and increases the time step size by 10% otherwise. As the growth process progresses, the time step size decreases initially and then increases. The minimum time step size of $\Delta t^{\min} = 0.020$ at a surface growth multiplier of $\hat{\vartheta} = 1.13$ corresponds exactly to the onset of buckling, when the five perturbations transition from an initially convex to an inward folded concave state.

Fig. 8 illustrates surface growth of inner tubular surface at the discrete time points summarized in Table 2. The upper and lower rows display the spatio-temporal evolution of the radial and deviatoric stresses. As time progresses, the growing inner surface successively increases in area, pulling the elastic bulk inward. During this growth process, the pentagonal perturbation grows into five distinct inner folds. Both radial and deviatoric stresses display significant regional variations. While radial stresses are primarily concentrated in convex regions where the volume is stretched most, deviatoric stresses are concentrated mainly in concave regions where the volume is compressed most.

Table 2
Algorithmic performance. Quadratic convergence of the surface growth model.

$\hat{\vartheta}$	1.00	1.25	1.50	2.00	2.75
Step 1	1.0000E+00	1.0000E+00	1.0000E+00	1.0000E+00	1.0000E+00
Step 2	1.8604E−02	1.7340E−01	1.0223E−01	7.9276E−02	5.6364E−02
Step 3	5.4821E−05	2.8761E−03	5.9689E−04	8.4273E−04	4.6647E−04
Step 4	1.1918E−08	8.3465E−07	2.8874E−08	2.0194E−07	6.0808E−08
Step 5	6.9602E−14	1.6881E−13	6.5397E−14	1.5026E−13	5.9122E−14
t	0.100	0.885	1.892	4.117	8.536
Δt	0.100	0.057	0.149	0.351	0.753

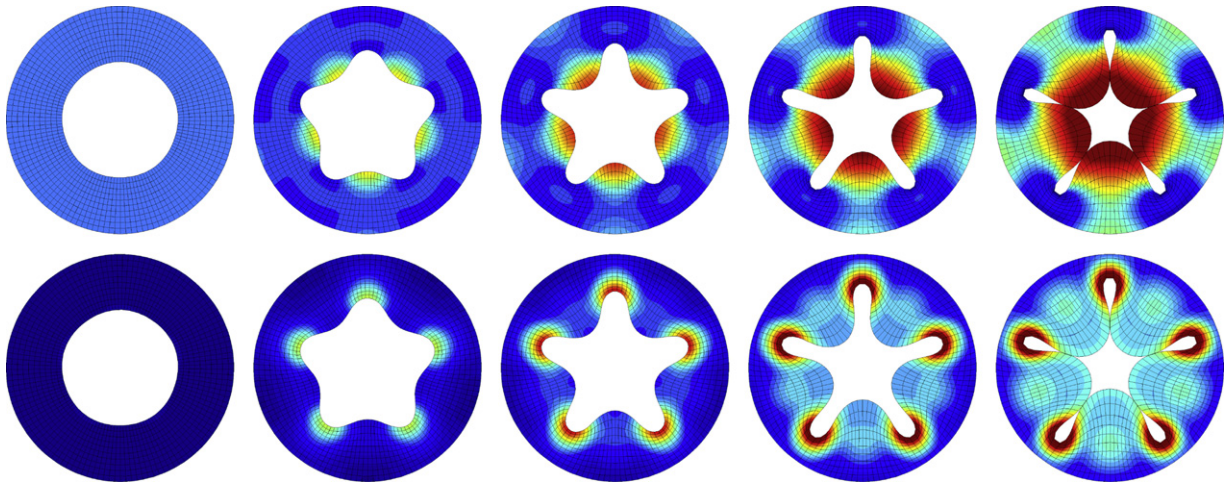


Fig. 8. Surface growth of inner surface of a cylindrical tube with pentagonally perturbed inner surface. Spatio-temporal evolution of radial stresses, top, and deviatoric stresses, bottom. The growing inner surface successively increases in area, pulling the elastic volume inward. As growth progresses, the pentagonal perturbation grows into five distinct inner folds. Snapshots correspond to $\hat{\vartheta} = 1.00$, $\hat{\vartheta} = 1.25$, $\hat{\vartheta} = 1.50$, $\hat{\vartheta} = 2.00$, and $\hat{\vartheta} = 2.70$.

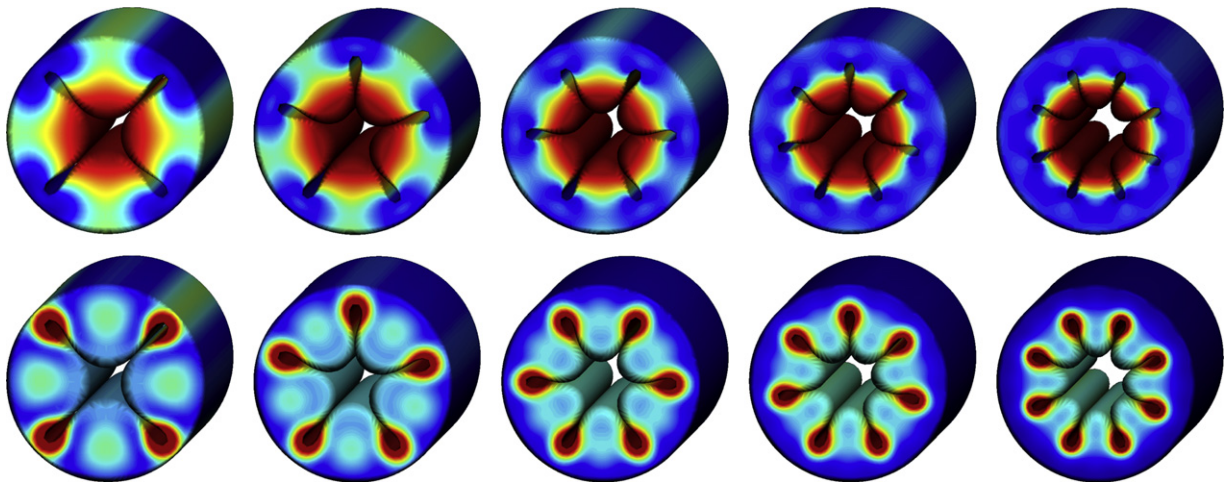


Fig. 9. Surface growth of inner surface of a cylindrical tube with perturbed inner surface. Spatial distribution of radial stresses, top, and deviatoric stresses, bottom. Square, pentagonal, hexagonal, heptagonal, and octagonal perturbations transition into four, five, six, seven, and eight distinct inner folds. Snapshots correspond to the time point of first self contact, which occurs consistent at $\hat{\vartheta} = 2.70$ for all perturbations.

Fig. 9 provides a fully three-dimensional view of the surface growth process. To explore the impact of the degree of perturbation, we systematically vary the number of perturbations applied to the inner surface. Square, pentagonal, hexagonal, heptagonal, and octagonal perturbations, displayed from left to right, gradually transition into four, five, six, seven, and eight distinct inner folds. The upper and lower rows display the spatial distribution of the radial and deviatoric

stresses. Both stress patterns are conceptually similar for different degrees of perturbation, displaying maximum radial stresses in convex regions where the volume is stretched most, and maximum deviatoric stresses in concave regions where the volume is compressed most. The illustrated snapshots correspond to the time point of first self-contact, which occurs consistent at $\hat{\vartheta} = 2.75$ for all five perturbations.

7. Discussion

Growth in constrained geometries is an important phenomenon of equal relevance to material sciences, biology, and medicine. Here, we have compared two conceptually different types of growth: classical volume growth, which has been explored intensely within the past decade; and surface growth, which has been realized using the concept of continua with boundary energies. While volume growth can reasonably well model biological systems of finite thickness, surface growth is appropriate to characterize phenomena at the zero thickness limit. Our new continuum framework for growing surfaces is therefore particularly appealing for growing thin films and growing biological linings of several cell layers.

In this manuscript, we have established the kinematic equations, the balance equations, and the constitutive equations for continua with boundary energies and growing surfaces. To motivate this novel concept, we have derived all sets of equations in complete analogy to continua with growing volumes. We have discretized the underlying weak forms and illustrated their consistent algorithmic linearization. To systematically compare growing volumes and growing surfaces, we have simulated constrained growth of finite-thickness and zero-thickness linings of a hyperelastic cylindrical tube.

Figs. 6–9 have shown that both volume and surface growth are capable of predicting extreme growth of the inner cylindrical lining, which more than doubled its initial area throughout the growth process. Both algorithms are robust and stable to simulate growth during the onset of buckling and beyond. Simulating the initiation of buckling instabilities is numerically highly challenging. To address this issue, we have adopted an ad hoc time adaptive scheme, which automatically reduces the time step size during phases when the Newton Raphson iteration does not converge within a limited number of iteration steps. This time adaptation has proven crucial to accurately track the initial stage of the instability and efficiently simulate growth beyond this critical point. However, this ad hoc adaptation scheme critically relies on a correct algorithmic linearization of the underlying highly nonlinear system of equations, which we have demonstrated through the characteristic quadratic convergence of the algorithmic residual in Tables 1 and 2.

To quantitatively compare volume and surface growth, Fig. 10 demonstrates the algorithmic performance of both formulations in terms of the adaptive time step size Δt . The blue, turquoise, green, orange, and red curves correspond to the square, pentagonal, hexagonal, heptagonal, and octagonal perturbations displayed in Figs. 7 and 9. With our particular time adaptive scheme, the required time step sizes for volume growth, left, were 0.002, 0.003, 0.004, 0.006, and 0.009 for the five simulations. The required time step sizes for surface growth, right, were 0.022, 0.020, 0.030, 0.030, and 0.025, i.e., they were in average an order of magnitude larger. Fig. 11 compares both formulations in terms of the growth multiplier $\hat{\vartheta}$. The algorithm for volume growth, left, required 187, 154, 131, 114, and 98 simulation steps toward the point of first self contact, shown in Fig. 7, while the algorithm for surface growth, right, required only 47, 47, 40, 41, and 42 steps toward this point, shown in Fig. 9. Although these numbers strongly depend on the particular choice and parameterization of the

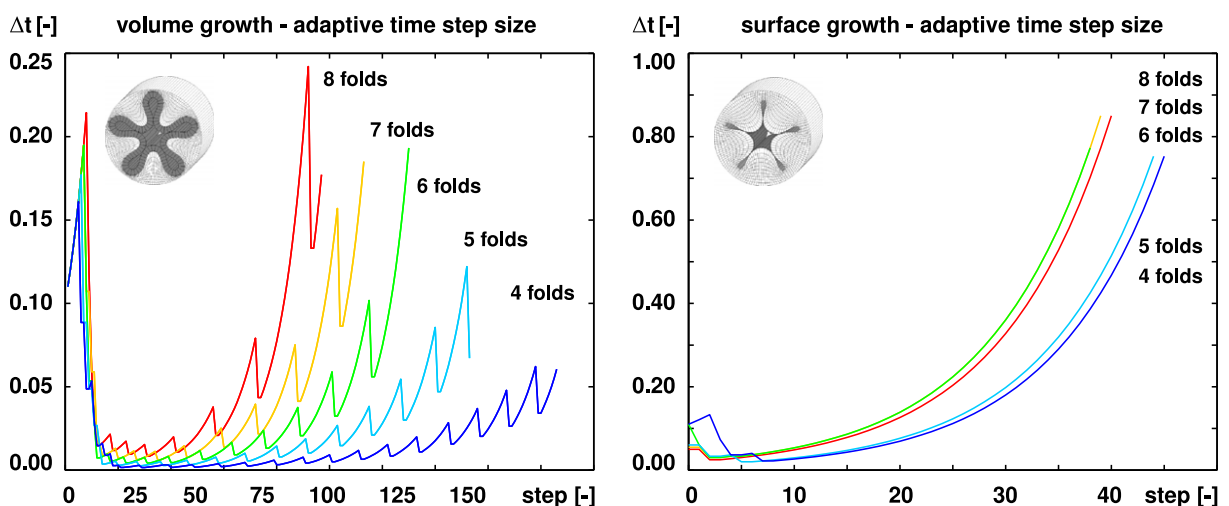


Fig. 10. Algorithmic performance. Evolution of adaptive time step size Δt for volume growth, left, and surface growth, right. The blue, turquoise, green, orange, and red curves correspond to the square, pentagonal, hexagonal, heptagonal, and octagonal perturbations displayed in Figs. 7 and 9. The algorithm for volume growth requires significantly smaller time step sizes than the algorithm for surface growth. (For interpretation of the references to color in this figure caption, the reader is referred to the web version of this article.)

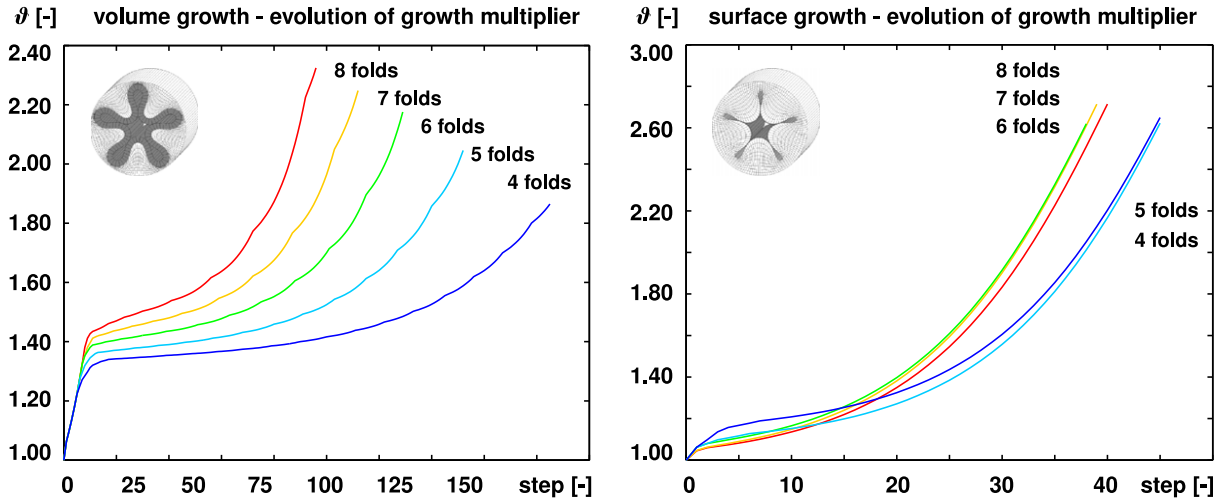


Fig. 11. Algorithmic performance. Evolution of growth multiplier θ for volume growth, left, and surface growth, right. The blue, turquoise, green, orange, and red curves correspond to the square, pentagonal, hexagonal, heptagonal, and octagonal perturbations displayed in Figs. 7 and 9. The algorithm for volume growth requires significantly more simulation steps toward the point of first self contact than the algorithm for surface growth.

time adaptation scheme, these studies indicate that surface growth is computationally more robust and more efficient than volume growth.

The present formulation for continua with boundary energies and growing surfaces is particularly suited to model phenomena, in which the thickness of the growing membrane is significantly smaller than the overall dimensions of the system (Gurtin and Murdoch, 1975). The thickness of the mucous membrane is typically less than a millimeter (Moulton and Goriely, 2011), the thickness of the cerebral cortex of the brain is of the order of millimeters (Wyczalkowski et al., 2012), the thickness of the epidermis of skin is of the order of several cell layers (Buganza Tepole et al., 2011). During growth, neither the cortical (Xu et al., 2010) nor the epidermal (Zöllner et al., 2012a) thicknesses undergo relevant changes, while their surfaces may grow significantly. While the proposed theory is well suited for thin biological membranes close to the zero thickness limit, which do not grow considerably in the thickness direction, volume growth with different growth multipliers in plane and out of plane (Goriely and BenAmar, 2005; Moulton and Goriely, 2011) might be more appropriate for thickening membranes. The role of thickness changes has been studied intensely in the context of mucosal folding (Wiggs et al., 1997). Parametric studies focus on identifying critical thickness ratios (Jin et al., 2011), stiffness ratios (Li et al., 2011), and growth multipliers (Li et al., 2011) at the onset of wrinkling. Another group of studies attributes the onset of buckling to an increased muscular pressure at the outer surface and focuses on identifying critical pressure-to-luminal-areal (Wiggs et al., 1997) or critical pressure-to-growth (Moulton and Goriely, 2011) curves. While we have limited the current examples to growth-induced instabilities, we plan to investigate the impact of pressure-induced instabilities in the near future. Another limitation of the proposed approach is that the evolution of growth is prescribed constitutively through Eqs. (35) and (44) as illustrated in Fig. 3. Replacing the morphogenetically driven growth law by a mechanically driven growth law is conceptually possible. However, the corresponding linearization will become slightly more cumbersome, as we have recently shown in the context of volume growth (Göktepe et al., 2010; Zöllner et al., 2012).

8. Conclusion

Many biological systems are coated by thin films, which display a fundamentally different behavior than the bulk. Here we have explored the physics and the numerics for growing thin biological surfaces. To model surface growth and the associated kinematic instabilities, we have compared two alternative concepts, classical volume growth for systems with a finite thickness and surface growth for systems with a zero thickness. Although the growing surfaces of both formations may look kinematically similar, aside from the underlying physics, there are three essential differences between the two schemes: First, and most obvious, surface growth is kinematically more localized than volume growth. It affects only the area of the inner lining, whereas volume growth also affects the thickness of the growing layer. Second, surface growth induces smoother stress profiles than volume growth. Its stresses are not just concentrated in the growing layer, but are distributed smoothly throughout the entire hyperelastic bulk. This implies that the peak stresses during surface growth are significantly smaller. This difference might become relevant in surface debonding, since elevated peak stresses are a hallmark for interface failure and an important indicator for layer separation. Third, surface growth is algorithmically more robust than volume growth. Surface growth accurately captures the onset of instabilities and traces the equilibrium path efficiently. Under the same conditions, the simulation of growing surfaces is about an order of magnitude faster than the simulation of growing volumes.

We believe that the concept of continua with boundary energies and growing surfaces will be widely applicable to predict growth-induced morphological instabilities in thin biological membranes, and, ultimately, support the design of new diagnostic tools and therapies for various types of respiratory, digestive, and urogenital disorders such as asthma, bronchitis, gastritis, obstructive sleep apnoea, and tumor invasion. In addition, the fundamental scientific understanding of growth-induced morphological instabilities has important implications in material sciences, manufacturing, and micro-fabrication, and may support the rational design of smart materials with tunable patterns and functional surfaces in soft lithography, metrology, and flexible electronics.

Acknowledgments

This study was supported by the National Science Foundation CAREER award CMMI 0952021 and INSPIRE Grant 1233054 and by the National Institutes of Health Grant U54 GM072970.

References

- Ambrosi, D., Mollica, F., 2002. On the mechanics of a growing tumor. *Int. J. Eng. Sci.* 40, 1297–1316.
- Ambrosi, D., Ateshian, G.A., Arruda, E.M., Cowin, S.C., Dumais, J., Goriely, A., Holzapfel, G.A., Humphrey, J.D., Kerkemer, R., Kuhl, E., Olberding, J.E., Taber, L.A., Garikipati, K., 2011. Perspectives on biological growth and remodeling. *J. Mech. Phys. Solids* 59, 863–883.
- Ben Amar, M., Goriely, A., 2005. Growth and instability in elastic tissues. *J. Mech. Phys. Solids* 53, 2284–2319.
- Buganza Tepole, A., Ploch, C.J., Wong, J., Gosain, A.K., Kuhl, E., 2011. Growing skin – a computational model for skin expansion in reconstructive surgery. *J. Mech. Phys. Solids* 59, 2177–2190.
- Buganza Tepole, A., Gosain, A.K., Kuhl, E., 2012. Stretching skin: the physiological limit and beyond. *Int. J. Nonlinear Mech.* 47, 938–949.
- Cao, Y.P., Li, B., Feng, X.Q., 2012. Surface wrinkling and folding of core-shell soft cylinders. *Soft Matter* 8, 556–562.
- Davies, D.E., Wicks, J., Powell, R.M., Puddicombe, S.M., Holgate, S.T., 2003. Airway wall remodeling in asthma: new insights. *J. Allergy Clin. Immunol.* 111, 215–225.
- Dervaux, J., Ciarletta, P., Ben Amar, M., 2009. Morphogenesis of thin hyperelastic plates: a constitutive theory of biological growth in the Föppl-von Karman limit. *J. Mech. Phys. Solids* 57, 458–471.
- Dervaux, J., Ben Amar, M., 2011. Buckling considerations in constrained growth. *J. Mech. Phys. Solids* 59, 538–560.
- Epstein, M., Maugin, G.A., 2000. Thermomechanics of volumetric growth in uniform bodies. *Int. J. Plast.* 16, 951–978.
- Garikipati, K., 2009. The kinematics of biological growth. *Appl. Mech. Rev.* 62, 030801.1–030801.7.
- Göktepe, S., Abilez, O.J., Parker, K.K., Kuhl, E., 2010. A multiscale model for eccentric and concentric cardiac growth through sarcomerogenesis. *J. Theor. Biol.* 265, 433–442.
- Göktepe, S., Abilez, O.J., Kuhl, E., 2010. A generic approach towards finite growth with examples of athlete's heart, cardiac dilation, and cardiac wall thickening. *J. Mech. Phys. Solids* 58, 1661–1680.
- Goriely, A., Ben Amar, M., 2005. Differential growth and instability in elastic shells. *Phys. Rev. Lett.* 94, 198103.
- Gurtin, M.E., Murdoch, A., 1975. A continuum theory of elastic material surfaces. *Arch. Ration. Mech. Anal.* 57, 291–323.
- Gurtin, M.E., Struthers, A., 1990. Multiphase thermomechanics with interfacial structure. *Arch. Ration. Mech. Anal.* 112, 97–160.
- Himpel, G., Kuhl, E., Menzel, A., Steinmann, P., 2005. Computational modeling of isotropic multiplicative growth. *Comput. Mod. Eng. Sci.* 8, 119–134.
- Hogg, J., 2004. Pathophysiology of airflow limitation in chronic obstructive pulmonary disease. *Lancet* 364, 709–721.
- Javili, A., Steinmann, P., 2009. A finite element framework for continua with boundary energies. Part I: the two-dimensional case. *Comput. Meth. Appl. Mech. Eng.* 198, 2198–2208.
- Javili, A., Steinmann, P., 2010. A finite element framework for continua with boundary energies. Part II: the three-dimensional case. *Comput. Meth. Appl. Mech. Eng.* 199, 755–765.
- Javili, A., Steinmann, P., 2010. On thermomechanical solids with boundary structures. *Int. J. Solids Struct.* 47, 3245–3253.
- Javili, A., Steinmann, P., 2011. A finite element framework for continua with boundary energies. Part III: the thermomechanical case. *Comput. Meth. Appl. Mech. Eng.* 200, 1963–1977.
- Jin, L., Cai, S., Suo, Z., 2011. Creases in soft tissues generated by growth. *EPL Front. Phys.* 95, 64002.1–64002.6.
- Kairaitis, K., 2012. Pharyngeal wall fold influences on the collapsibility of the pharynx. *Med. Hypotheses* 79, 327–376.
- Kroon, W., Delhaas, T., Arts, T., Bovendeerd, P., 2009. Computational modeling of volumetric soft tissue growth: application to the cardiac left ventricle. *Biomech. Model. Mechanobiol.* 8, 309–310.
- Kuhl, E., Steinmann, P., 2003a. Mass- and volume specific views on thermodynamics for open systems. *Proc. R. Soc.* 459, 2547–2568.
- Kuhl, E., Steinmann, P., 2003b. On spatial and material settings of thermohyperelastodynamics for open systems. *Acta Mech.* 160, 179–217.
- Kuhl, E., Maas, R., Himpel, G., Menzel, A., 2007. Computational modeling of arterial wall growth: attempts towards patient-specific simulations based on computer tomography. *Biomech. Mod. Mechanobiol.* 6, 321–331.
- Kuhl, E., Schmid, D.W., 2007. Computational modeling of mineral unmixing and growth: an application of the Cahn–Hilliard equation. *Comput. Mech.* 39, 439–451.
- Laplace, P.S., 1805. *Traité de Mécanique Céleste. Oeuvres complètes*, Vol. 4, Suppl. 1, Livre X:771–777. Gauthier-Villars, Paris.
- Lee, E.H., 1969. Elastic-plastic deformation at finite strains. *J. Appl. Mech.* 36, 1–6.
- Lee, M.M.L., Chien, S., 1978. Morphologic effects of pressure changes on canine carotid artery endothelium as observed by scanning electron microscopy. *Anat. Rec.* 194, 1–14.
- Leo, P.H., Sekerka, R.F., 1989. The effect of surface stress on crystal-melt and crystal-crystal equilibrium. *Acta Metall.* 37, 3119–3138.
- Leo, P.H., Sekerka, R.F., 1989. The effect of elastic fields on the morphological stability of a precipitate grown from solid solution. *Acta Metall.* 37, 3139–3149.
- Li, B., Cao, Y.P., Feng, X.Q., Gao, H., 2011. Surface wrinkling of mucosa induced by volumetric growth: theory, simulation and experiment. *J. Mech. Phys. Solids* 59, 758–774.
- Li, B., Cao, Y.P., Feng, X.Q., Yu, S.W., 2011. Mucosal wrinkling in animal antra induced by volumetric growth. *Appl. Phys. Lett.* 98, 153701.
- Li, B., Cao, Y.P., Feng, X.Q., Gao, H., 2012. Mechanics of morphological instabilities and surface wrinkling in soft materials: a review. *Soft Matter* 8, 5728–5745.
- Liao, D., Zhao, J., Gregersen, H., 2007. The oesophageal zero-stress state and mucosal folding from a GIOME perspective. *World J. Gastroenterol.* 13, 1347–1351.
- McBride, A.T., Javili, A., Steinmann, P., Bargmann, S., 2011. Geometrically nonlinear continuum theories with surface energies coupled to diffusion. *J. Mech. Phys. Solids* 59, 2116–2133.
- McMahon, J., Goriely, A., 2010. Spontaneous cavitation in growing elastic membranes. *Math. Mech. Solids* 15, 57–77.

- Menzel, A., 2005. Modelling of anisotropic growth in biological tissues – a new approach and computational aspects. *Biomech. Model. Mechanobiol.* 3, 147–171.
- Menzel, A., Kuhl, E., 2012. Frontiers in growth and remodeling. *Mech. Res. Comm.* 42, 1–14.
- Moulton, D.E., Goriely, A., 2011. Circumferential buckling instability of a growing cylindrical tube. *J. Mech. Phys. Solids* 59, 525–537.
- Moulton, D.E., Goriely, A., 2011. Possible role of differential growth in airway wall remodeling in asthma. *J. Appl. Physiol.* 110, 1003–1012.
- Nelson, M.R., Howard, D., Jensen, O.E., King, J.R., Rose, F.R.A.J., Waters, S.L., 2011. Growth-induced buckling of an epithelial layer. *Biomech. Model. Mechanobiol.* 10, 883–900.
- Pare, P.D., McParland, B.E., Seow, C.Y., 2007. Structural basis for exaggerated airway narrowing. *Can. J. Physiol. Pharmacol.* 85, 653–658.
- Rausch, M.K., Dam, A., Göktepe, S., Abilez, O.J., Kuhl, E., 2011. Computational modeling of growth: systemic and pulmonary hypertension in the heart. *Biomech. Model. Mechanobiol.* 10, 799–811.
- Rausch, M.K., Tibayan, F.A., Miller, D.C., Kuhl, E., 2012. Evidence of adaptive mitral leaflet growth. *J. Mech. Behav. Biomed. Mat.* 15, 208–217.
- Rodriguez, E.K., Hoger, A., McCulloch, A.D., 1994. Stress-dependent finite growth in soft elastic tissues. *J. Biomech.* 27, 455–467.
- Saksono, P.H., Peric, D., 2006. On finite element modelling of surface tension variational formulation and applications. Part I: quasistatic problems. *Comp. Mech.* 38, 251–263.
- Simha, N.K., Bhattacharya, K., 1998. Kinetics of phase boundaries with edges and junctions. *J. Mech. Phys. Solids* 46, 2323–2359.
- Simha, N.K., Bhattacharya, K., 2000. Kinetics of phase boundaries with edges and junctions in a three-dimensional multi-phase body. *J. Mech. Phys. Solids* 48, 2619–2641.
- Socci, L., Rennati, G., Gervaso, F., Vena, P., 2007. An axisymmetric computational model of skin expansion and growth. *Biomech. Model. Mechanobiol.* 6, 177–188.
- Steinmann, P., 2008. On boundary potential energies in deformational and configurational mechanics. *J. Mech. Phys. Solids* 56, 772–800.
- Suo, Z., 1997. Motions of microscopic surfaces in materials. *Adv. Appl. Mech.* 33, 193–294.
- Taber, L.A., 1995. Biomechanics of growth, remodeling and morphogenesis. *Appl. Mech. Rev.* 48, 487–545.
- Taber, L.A., Humphrey, J.D., 2001. Stress-modulated growth, residual stress, and vascular heterogeneity. *J. Biomech. Eng.* 123, 528–535.
- Tsamis, A., Cheng, A., Nguyen, T.C., Langer, F., Miller, D.C., Kuhl, E., 2012. Kinematics of cardiac growth – in vivo characterization of growth tensors and strains. *J. Mech. Behav. Biomed. Mat.* 8, 165–177.
- Vandiver, R., Goriely, A., 2009. Differential growth and residual stress in cylindrical elastic structures. *Phil. Trans. R. Soc. A* 367, 3607–3630.
- Wiggs, B.R., Hrousis, C.A., Drazen, J.M., Kamm, R.D., 1997. On the mechanism of mucosal folding in normal and asthmatic airways. *J. Appl. Physiol.* 83, 1814–1821.
- Wyczalkowski, M.A., Chen, Z., Filas, B.A., Varner, V.D., Taber, L.A., 2012. Computational models for mechanics of morphogenesis. *Birth Defects Res. C* 96, 132–152.
- Xu, G., Knutsen, A.K., Dikranian, K., Kroenke, C.D., Bayly, P.V., Taber, L.A., 2010. Axons pull on the brain, but tension does not drive cortical folding. *J. Biomech. Eng.* 132 (7), 071013.
- Young, T., 1805. An essay on the cohesion of fluids. *Phil. Trans. R. Soc. London* 95, 65–87.
- Zöllner, A.M., Buganza Tepole, A., Kuhl, E., 2012. On the biomechanics and mechanobiology of growing skin. *J. Theor. Biol.* 297, 166–175.
- Zöllner, A.M., Buganza Tepole, A., Gosain, A.K., Kuhl, E., 2012a. Growing skin – tissue expansion in pediatric forehead reconstruction. *Biomech. Mod. Mechanobiol.* 11, 855–867.
- Zöllner, A.M., Abilez, O.J., Böhl, M., Kuhl, E., 2012b. Stretching skeletal muscle: chronic muscle lengthening through sarcomerogenesis. *PLoS ONE* 7 (10), e45661.