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B A C H E L O R ' S   T H E S I S

# Modeling Calcium Dynamics in T Cells

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## **Acknowledgement**



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# 1. Introduction

As part of the bodies' defence against viruses t cells can undergo activation in their lifetime. Whether and when a t cell activates is an interesting topic when studying immunology. However, measuring activation is often done indirectly by using the correlation between calcium concentration within the cell and activation. Measuring the calcium concentration leads to a time series that can be analysed by experts for activation.

This work aims to provide an algorithm for automatic detection of activation. By using approximation algorithms the time series is fitted with sigmoid functions. This reduces the data from hundreds of values in a time series to few parameters of the approximation function. Additionally, the parameters are chosen to be valuable for interpretation by experts. This parameter representation of the data is then filtered and used for clustering the data into activated and unactivated cells.

The provided algorithm can be used on any data set provided a positive control and negative control is provided. The most simple use case of finding the number of activated cells in the data set is described in more detail.

The proposed algorithm is tested with two of the most common types of t cells, human Jurkat cells and mouse 5c.c7 cells.

The main question this work aims to answer is which criteria can distinguish between unactivated and activated cells. Additionally, a criterion for detecting cells which activated before the experiment began will be investigated.

When only looking at activated cells some interesting questions are whether there are different types of activated cells and how they are different. A typical pattern observed in activated cells is that they show oscillations of the calcium concentration. Analysing the frequencies of these oscillations might be interesting.

Lastly differences between mouse and human cells show whether the proposed algorithm is applicable to the two most common types of t cells studied.

To summarize the questions are

- Which criteria can distinguish between unactivated, activated and pre-activated cells?
- Do different types of activated cells exists? How are they different?
- With which frequencies does the Calcium concentration repeat after activation?
- Is there a difference between mouse and human cells?

with the first question being the most relevant.

This work starts with a chapter on optimization algorithms. In chapter 2 the relevant algorithm, Trust Region Reflective Algorithm, is attained from other algorithms, which are described as well.

Following is chapter 3 focusing on the biology of t cells. All relevant components of t cells for changes in calcium concentration are described. Their interconnections are described.

Next chapter 4 describes the structure and experimental setup for retrieving the data. Some processing steps performed on the data are outlined.

The main focus of this work, approximating the calcium concentration, are described in chapter 5. Here the approximation function is inferred and described. Parameter descriptions are provided. Pseudocode for the approximation algorithms are given and described. The parameters found from the approximation of the data sets used in this work are analysed. Oscillations are approximated in this chapter as well.

In chapter 6 the clustering algorithms Gaussian Mixture Model and KMeans are described and applied to the output of the approximation. Visual representation of the clustering is shown.

Chapter 7 aims to answer the questions posed above by using the approximation and clustering described in the other chapters.

A final discussion of the results provided in this work is provided in chapter 8. The outlook is featured here as well.

## 2. Optimization Algorithm

An optimization problem is any problem where a function  $f : X \rightarrow Y$  is given, and we search for the point  $x \in X$  such that  $f(x)$  is minimal or maximal. Obviously the minimum or maximum must not exist, as the example  $f : (0, 1) \rightarrow \mathbb{R}, x \mapsto x$  demonstrates by not having either. Investigating conditions on  $X, Y$  and  $f$  such that a minimum or maximum exists is mathematically interesting. However, when implementing an optimization algorithm the true minimum or maximum can sometimes not be found even if it exists and is instead replaced by a sufficiently good approximation.

### 2.1. Gradient Descent

An iterative algorithm for finding the minimum of a differentiable function  $f : \mathbb{R}^n \rightarrow \mathbb{R}$  is gradient descent. As the name suggests it uses information of the gradient  $\nabla f$ . Locally the negative gradient always points into the direction of greatest descent. The idea is to follow this direction for the next guess of the minimum. The pseudocode of this approach is given below.

---

**Algorithm 1:** Gradient Descent

---

```
input  :  $f : \mathbb{R}^n \rightarrow \mathbb{R}$  ... differentiable,  $x_0 \in \mathbb{R}^n$   
output:  $x \in \mathbb{R}^n$   
  
1 begin  
2   for  $n = 0$  to  $max\_iterations$  do  
3     if improvement is smaller than threshold then  
4       break  
5     end  
6     set or calculate step size  $\gamma_n$   
7      $x_{n+1} = x_n - \gamma_n \nabla f(x_n)$   
8   end  
9    $x = x_n$   
10 end
```

---

If we consider a function with a local minimum, that is not a global minimum, gradient descent might not converge to the optimum. An example of such a function can be seen in figure 2.1 along with the first few values  $x_n$  of gradient descent. The starting value was chosen to not have convergence to the global minimum. For a different starting value the global minimum can be reached.

Improvements can be made by choosing good step sizes, starting value or by starting



Figure 2.1.: The function has two local minimums. For this starting value and step size gradient descent approaches the local, but not global minimum.

with different values and comparing the results.

## 2.2. Least Square Problem Algorithms

We now focus on the Least Square Problem and give an introduction into various algorithms solving this problem.

In the example dealt with in this work we are given some data points  $((x_k, y_k))_{k \in \{1, 2, \dots, n\}}$  and want to find a close approximation in the form of a function  $g(x, a_1, a_2, \dots, a_m)$  where for every list of function parameters  $a = (a_1, \dots, a_m)$  we have the function  $g_a(x) : \mathbb{R} \rightarrow \mathbb{R}, x \mapsto g(x, a_1, \dots, a_m)$ . Searching for a good approximation can be reformulated as searching for the minimum of  $r(a) := \sum_{k=1}^n |g_a(x_k) - y_k|^2$  or any other error function. This form of optimization problem is called the Least Square Problem.

First we want to discuss some variations of the problem. Easiest to solve are linear problems. These can be formulated as the minimization of  $\|Ax - b\|^2$ , and solved using calculus by  $x = (A^T A)^{-1} A^T b$  provided the rank of  $A$  is full.

Often we want to constrain the search for a minimum under some properties. For linear problems we can find a formulation as

$$\text{minimize } \|Ax - b\|^2 \text{ subject to } Cx = d.$$

Finding a solution can be done by minimizing  $\|Ax - b\|^2 + \lambda \|Cx - d\|^2$  for very large  $\lambda$ .

General least square problems are formally given as a residual function  $r_f(x)$  which tells us whether a function  $f$  is a good approximation at the point  $x$ . We therefore want to find a way to minimize  $\|r_f(x)\|^2$ .

As  $\|r_f(x)\|^2 \geq 0$  we can turn to the simpler problem of finding a root. However, a root must not exist, in which case we want to find the value closest to zero. This is then the minimum of the function.

Some algorithm for minimization are now discussed below.

### 2.2.1. Gauss–Newton Algorithm

The idea behind this algorithm is that it is easy to find the intersection with zero of a linear function. If we linearize  $r : \mathbb{R}^n \rightarrow \mathbb{R}^m$  locally, we can approximate the root by finding it of the linear approximating function. This is demonstrated in figure 2.2.

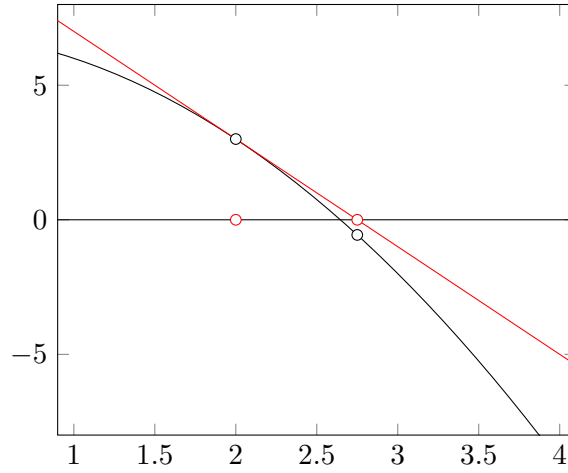


Figure 2.2.: By approximating the black function by a line an approximation of the root has been found.

Iterating this step of linear approximating gives us the Gauss-Newton Method. In figure 2.3 we can see that indeed  $x_n$  seems to converge towards the root of the function.

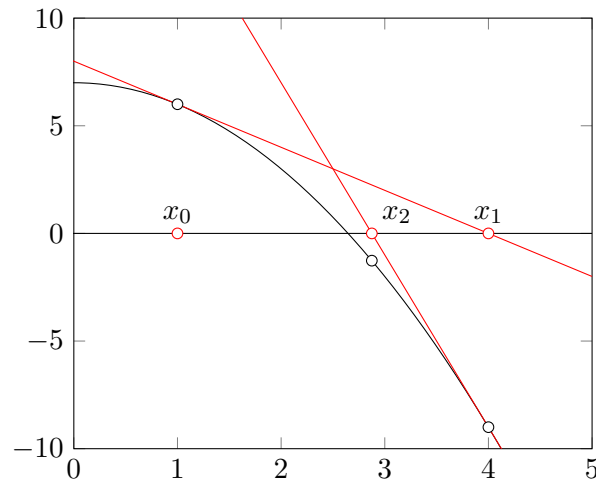


Figure 2.3.: Iteratively applying linear approximation gives the Gauss-Newton Method for approximating the root.

## 2. Optimization Algorithm

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Define  $Dr$  as the Jacobian matrix  $\left(\frac{\partial r_i}{\partial x_j}\right)_{ij}$ . Using Taylor's theorem we get the linear approximation

$$r(x) = r(a) + Dr(a)(x - a) + h(x)(x - a) \approx r(a) + Dr(a)(x - a) \text{ with } \lim_{x \rightarrow a} h(x) = 0.$$

Rewriting this as  $r(x) \approx Ax - b$  where  $A := Dr(a)$  and  $b := Dr(a)a - r(a)$  gives us the algorithm for this method. As  $Dr \in \mathbb{R}^{n \times m}$  we solve  $Dr^T Dr x = Dr^T b$  in order to get a system with square matrix. If  $n = m$  we can skip this step and get the so-called Newton algorithm as a variant.

---

**Algorithm 2:** Gauss-Newton

---

```
input :  $r : \mathbb{R}^n \rightarrow \mathbb{R}^m$  ... differentiable,  $x_0 \in \mathbb{R}^n$ 
output:  $x \in \mathbb{R}^n$ 

1 begin
2   for  $n = 0$  to  $max\_iterations$  do
3     if  $\|r(x_n)\|^2$  close enough to zero or  $\|x_n - x_{n-1}\|$  is too small then
4       break
5     end
6     Calculate  $A_n := Dr(x_n)$ 
7     Calculate  $b_n := A_n x_n - r(x_n)$ 
8     Solve  $A_n^T A_n x_{n+1} = A_n^T b_n$ 
9   end
10   $x := x_n$ 
11 end
```

---

Gauss-Newton is guaranteed to find a local minimum  $x$  if  $r$  is twice continuously differentiable in an open convex set including  $x$ ,  $Dr$  has a full rank and the initial value is close enough to  $x$ .

For the example demonstrated in figure 2.4 we can see that choosing a particular starting value leads to a loop in which only two points are explored as possible roots. More extreme examples exist in which Gauss-Newton gets increasingly further away from the root, due to an increasingly flat incline the further we get from the root. One example of such a function can be seen in figure 2.5.

Gauss-Newton has two problems, the starting value being too far from the root and  $Dr$  not having full rank. This can be combated using the technique of dampening. Instead of moving the new guess all the way to the root of the linear approximation we only move part of the way. How far to move can be determined by a dampening factor  $\lambda_n$  or a constant  $\lambda$ .

### 2.2.2. Levenberg-Marquardt Algorithm

This section is following section 18.3 of the book Introduction to Applied Linear Algebra by Stephen Boyd and Lieven Vandenbergh[Boyd2018].

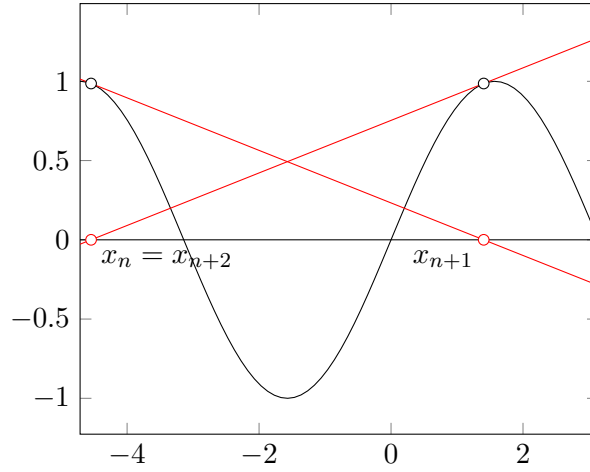


Figure 2.4.: For a poor choice of starting values Gauss-Newton can never find the root of the function  $\sin(x)$ .

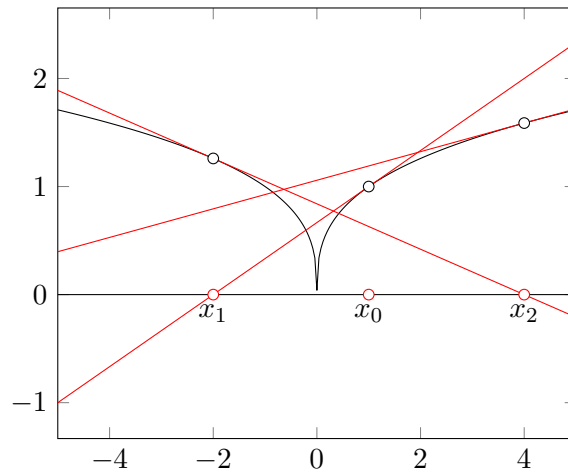


Figure 2.5.: Finding the root of the function  $\sqrt[3]{|x|}$  using Gauss-Newton is only possible if the starting value  $x_0$  is chosen as 0, which is the root. For any other value we have that the guess gets further and further away. Indeed for any  $x_n$  we have  $x_{n+1} = -2x_n$ .

## 2. Optimization Algorithm

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As stated above, a shortcoming of Gauss-Newton is that for  $x$  far from  $x_n$  we must not have that  $r(x) \approx r(x_n) + Dr(x_n)(x - x_n) =: \hat{r}(x, x_n)$ . Levenberg-Marquardt addresses this by minimizing  $\|\hat{r}(x, x_n)\|^2 + \lambda_n \|x - x_n\|^2$ . The first part is the same as above, while the second objective expresses our desire to not stray away too much from the region where we trust the linear approximation. The parameter  $\lambda_n$  is a positive parameter specifying how far the trusted region extends.

Writing the above idea as a single squared norm to minimize gives us the problem

$$\text{minimize } \left\| \begin{pmatrix} Dr(x_n) \\ \sqrt{\lambda_n} I \end{pmatrix} x - \begin{pmatrix} Dr(x_n)x_n - r(x_n) \\ \sqrt{\lambda_n} x_n \end{pmatrix} \right\|^2.$$

We observe that as  $\lambda_n$  is positive the left matrix has full rank. From this it follows that a unique solution exists.

The change of including  $\lambda_n$  translates into the algorithm as replacing solving  $A_n^T A_n x_{n+1} = A_n^T b_n$  in Gauss-Newton by solving  $A_n^T A_n z + \lambda_n z = A_n^T b_n + \lambda_n x_n$ .

The question of how to choose  $\lambda_n$  arises. If too small  $x_{n+1}$  can be too far from  $x_n$  to trust the approximation. If too big the convergence will be slow. If in the previous step the objective  $\|r(x_n)\|^2$  decreased we decrease  $\lambda_{n+1}$  slightly. If the last step was not successful  $\lambda_n$  was too small. Therefore we increase  $\lambda_{n+1}$ .

Pseudo code of the resulting Levenberg-Marquardt algorithm is shown below. The stopping criteria of  $\|2Dr(x_n)^T r(x_n)\|$  being too small is known as the optimality condition. It is derived from the fact that  $2Dr(x)^T r(x) = \nabla \|r(x)\|^2 = 0$  holds for any  $x$  minimizing  $\|r(x)\|^2$ . Note that this condition can be met for points other than the minimum.

---

### Algorithm 3: Levenberg-Marquardt

---

```

input :  $r : \mathbb{R}^n \rightarrow \mathbb{R}^m$  ... differentiable,  $x_0 \in \mathbb{R}^n$ ,  $\lambda_0 > 0$ 
output:  $x \in \mathbb{R}^n$ 

1 begin
2   for  $n = 0$  to  $max\_iterations$  do
3     Calculate  $A_n := Dr(x_n)$ 
4     Calculate  $b_n := A_n x_n - r(x_n)$ 
5     if  $\|r(x_n)\|^2$  close enough to zero or  $\|2A_n^T r(x_n)\|$  is too small then
6       break
7     end
8     Solve  $(A_n^T A_n + \lambda_n)z = A_n^T b_n + \lambda_n x_n$ 
9     if  $\|r(z)\|^2 < \|r(x_n)\|^2$  then
10       $x_{n+1} := z$ 
11       $\lambda_{n+1} := 0.8\lambda_n$ 
12    else
13       $x_{n+1} := x_n$ 
14       $\lambda_{n+1} := 2\lambda_n$ 
15    end
16  end
17   $x := x_n$ 
18 end

```

---



Coming back to the example where Gauss-Newton failed we once again consider the function from figure 2.5. In comparison this time we are able to find a good approximation of the root using Levenberg-Marquardt. A few steps are demonstrated in figure 2.6.

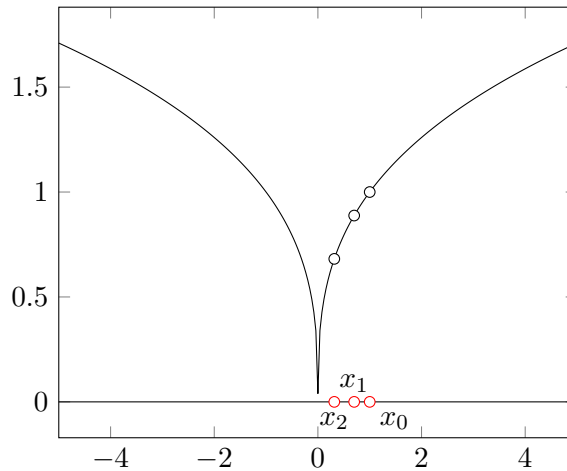


Figure 2.6.: In comparison to Gauss-Newton, Levenberg-Marquardt is able to find the root of the function  $\sqrt[3]{|x|}$ . From the starting value  $x_0 := 1$  and using  $\lambda_0 := 1$  the guesses  $x_n$  move towards the root  $x = 0$ .

Further improvements to this algorithm can be made using good starting values perhaps from the output of other algorithms or by letting the algorithm run multiple times with different starting values and comparing the results.

### 2.2.3. Algorithms for Bounded Least Square Problems

The algorithms described above do not consider bounds. For bounded problems two algorithms known as Trust Region Reflective Algorithm and Dogleg Algorithm with Rectangular Trust Regions can be used.

Trust Region Reflective gets its name from the use of trust regions as in Levenberg-Marquardt as well as reflecting along the bounds[branch1999]. If an iterative  $x_n$  lands outside the bounds set, it is replaced by a reflected value within the bounds. This ensures each iterative is feasible as a solution.

As the name suggests the Dogleg Algorithm with Rectangular Trust Regions uses rectangular trust regions as opposed to ellipsoids.[voglis2004] As the bounds are specified as a rectangle to stay within, this results in the intersection of trust region and bounds to be rectangular. The resulting minimizing problem is solved with an adequate algorithm[Nocedal1999].

In Python the library SciPy provides the three methods Levenberg-Marquardt, Trust Region Reflective and Dogleg with Rectangular Trust Regions for solving Least Square Problems.



### 3. Background Information on T Cells and Calcium Concentration

Lymphocytes form a key component of the immune system. T cells are a type of lymphocyte and are responsible for responding to viruses, fungi, allergens and tumours. Different subtypes of t cells exist, that perform various responsibilities. They are transported throughout the body via the lymphatic system and blood.[Kumar2018]

Precursor cells are formed in the bone marrow. Once they are transported to the thymus they undergo maturation and selection to become t cells. Each cell forms receptors, called t cell receptors (TCR), that respond to one particular out of many ( $10^6$ – $10^9$ ) possible short pieces of proteins, called peptides. These peptides are attached to the major histocompatibility complex (MHC) present on antigens and antigen presenting cells (APC). Important aspects of the selection are ensuring that the t cells react to foreign peptides, but not to those present on the body's own cells.[Ashby2024]

In positive selection, cells in the thymus present peptides on their MHC. If a t cell is unable to bind, it will undergo apoptosis, a type of cell death. T cells which were able to bind receive survival signals. Negative selection verifies that t cells will not attack the body's own cells. This is done by only selecting t cells which only bind moderately to the peptides presented, as a strong bond suggests that these t cells would have a high likelihood of being reactive to own cells.[Hagel2018] If a t cell passed both the positive and negative selection it is transported to the periphery.

There are multiple types of peripheral t cells. Native t cells respond to new antigens. Cytotoxic t cells kill cells which present peptides on their MHC compatible with the t cells TCR. Helper T cells activate other parts of the immune response. Memory t cells shorten the reaction time when the same antigen is encountered again at a later point in time. Suppressor t cells moderate the immune response.[Ganong1997]

#### 3.1. Components of a T Cell

T cell components relevant in activation and subsequent changes in intracellular  $\text{Ca}^{2+}$  are listed below.

- **T cell receptor (TCR):** Receptor on the cell surface that can recognize peptides. By the simultaneous triggering of the TCR and co-stimulator, signalling is induced that leads to activation.
- **Co-stimulator:** A stimulation of co-stimulatory molecules is necessary in order for signalling to occur as part of activation.

### 3. Background Information on T Cells and Calcium Concentration

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- **Endoplasmic reticulum (ER):** A series of connected sacs in the cytoplasm that is attached to the nucleus. Important functions are folding, modification and transportation of proteins.[Rogers2024]
- **Ca<sup>2+</sup> permeable ion channel on the ER:** There are several Ca<sup>2+</sup> channels present on the ER. Some receptors are responsible for releasing Ca<sup>2+</sup> into the cytoplasm, when the intracellular Ca<sup>2+</sup> concentration is low. [Schwarz2016]
- **Ca<sup>2+</sup> storage in the ER:** Ca<sup>2+</sup> is stored in the ER and can be released by Ca<sup>2+</sup> permeable ion channels on the ER.
- **Cytoplasm:** The semi-fluid substance enclosed in the plasm membrane. It contains organelles, ions, proteins and molecules.
- **Stromal interaction molecule (STIM):** If the Ca<sup>2+</sup> storage in the ER is depleted STIM proteins cluster where the ER is in the vicinity of the plasm membrane and assembles CRAC, which then leads to uptake in extracellular Ca<sup>2+</sup>. [Schwarz2016]
- **Plasm membrane:** A semipermeable structure forming the wall of the cell made up of lipids and proteins. Ion channels and transport proteins allow certain substances to move through.[Ganong2012]
- **Ca<sup>2+</sup> release activated Ca<sup>2+</sup> channel (CRAC):** Opened after a decrease in ER stored Ca<sup>2+</sup> is sensed by STIM, these channels intake Ca<sup>2+</sup> from outside the cell.[Stathopulos2013]
- **Cytoskeleton:** A system of fibres within the cell, that allows it to change shape and move.[Ganong2012]
- **Nucleus:** An organelle that stores most of the DNA, controls cell growth and cell division. A double membrane separates it from the cytoplasm.[cooper2022]

Relevant components of APC are the

- **Major histocompatibility complex (MHC)**, which can present peptides, and the
- **Co-stimulator**, which can form a bond with the co-stimulator on a t cell.

Both are present on the surface of the APC.

All components are schematically shown in figure 3.1.

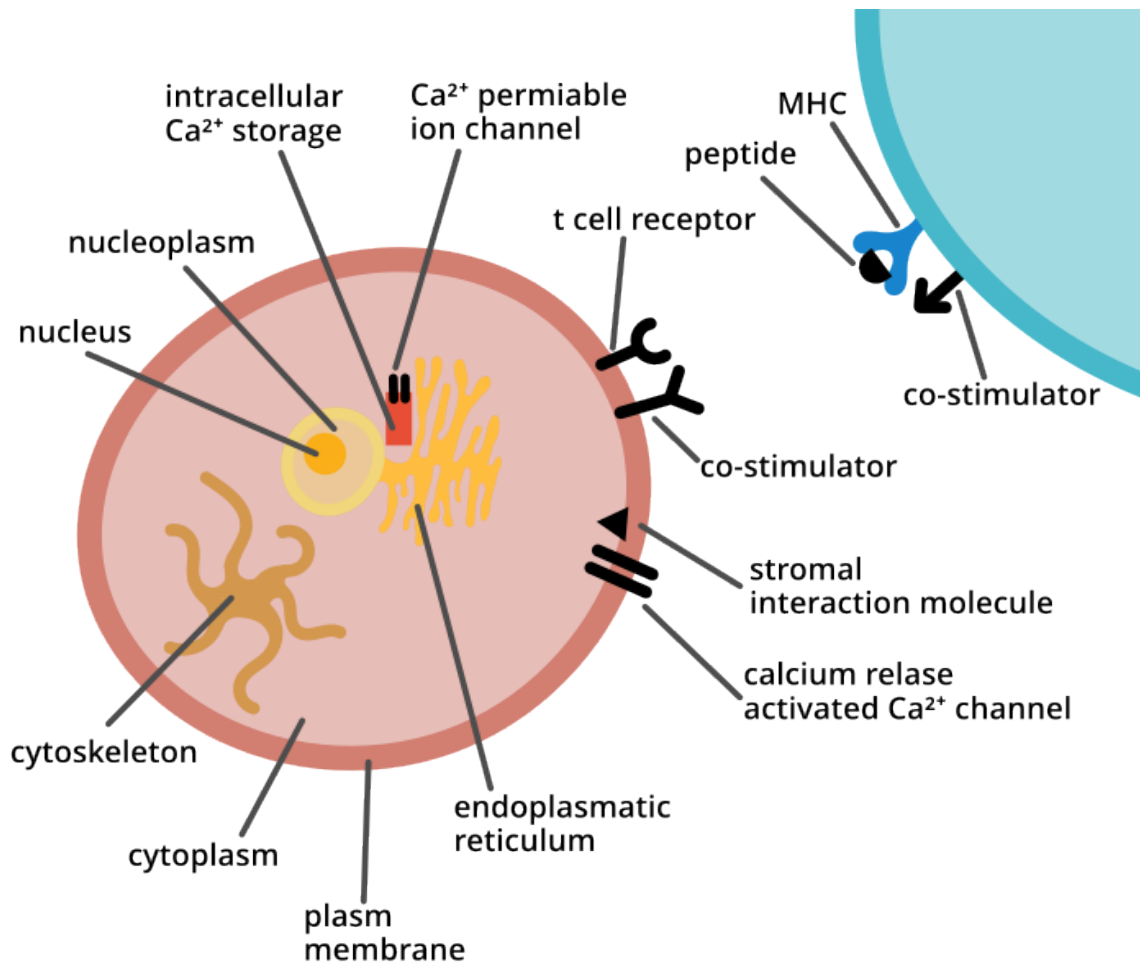


Figure 3.1.: Schematic view of a t cell and antigen presenting cell, with all relevant components.

### 3.2. Activation of T Cells

Activation is necessary for t cells to divide and perform their functions.[Ganong1997]

When a native t cell encounters a peptide on an APC that is compatible, a bond is formed between the TCR on the t cell and the peptide-MHC complex on the APC. This recognition can be triggered by less than ten molecules of foreign substance and is therefore described as near perfect. Sufficiently long contact is necessary between the APC and the t cell in order for the t cell to activate. The role of contact time in t cell activation is modelled by Morgan et al.[morgan2023].

The presence of co-stimulatory molecules is needed for activation. The bond between the co-stimulatory molecules on the t cell and the one on the APC plays a role in signalling. Especially  $\text{Ca}^{2+}$  signals play a vital part in t cell activation.

### 3. Background Information on T Cells and Calcium Concentration

---

An increase of  $\text{Ca}^{2+}$  in t cells during activation is caused by the stimulation of  $\text{Ca}^{2+}$  permeable ion channel receptors on the ER membrane.  $\text{Ca}^{2+}$  is released from the ER into the cytoplasm. Additionally, this decrease in  $\text{Ca}^{2+}$  is sensed by STIM, which leads to an influx of  $\text{Ca}^{2+}$  through plasma membrane CRAC channels.[**smith2009**]

As the intracellular  $\text{Ca}^{2+}$  concentration is dependent on the interaction between  $\text{Ca}^{2+}$  sources and sinks, a variety of different forms in  $\text{Ca}^{2+}$  concentration have been observed. Examples are infrequent spikes, sustained oscillations and plateaus.[**Lewis2001**]

Intercellular  $\text{Ca}^{2+}$  increase together with other signals lead to a redistribution of receptors, signalling molecules and organelles.[**joseph2014**]

## 4. Calcium Data of T Cells

From section 3.2, we gather that analysing the intracellular  $\text{Ca}^{2+}$  concentration gives us good insight in whether and when a cell activates. Additionally, it can be measured relatively easily by the method described in this chapter.

### 4.1. Structure of the Data

First we describe the structure of the data this work uses.

The data matrix has one row for each combination of tracked particle and frame number. In this context cells are called particles as the recording might feature non-cells that are detected as a cell and recorded in the data set. The information stored for each particle and frame combination is described in detail in 4.1.

Name	Data Type	Description
x	float64	Position of particle in pixels along the horizontal axis
y	float64	Position of particle in pixels along the vertical axis
frame	int32	Number of frame, with frame rate of 1 frame per second
mass short	float64	Brightness of cell in 340nm channel
mass long	float64	Brightness of cell in 380nm channel
ratio	float64	Calculated as mass short divided by mass long
particle	int32	Identification for each particle

Table 4.1.: Description and data type of all columns present in the data matrix.

One recording can have between 500 and 10000 particles and is between 700 and 1000 frames long, which corresponds to between about 11 and 17 minutes. The ratio recorded is typically between 0 and 5.

Four recordings were generated, with two each from human and mouse cells. For each cell type a positive and negative control was measured. In a positive control the conditions are such, that in theory every cell should activate, while in negative control the conditions are such, that none should activate. Due to stress on the cells caused by the movement or changes in temperature and other factors a few cells will activate before the recording starts, during the recording in the negative control or not activate at all in the positive control, regardless of the conditions.

### 4.2. Jurkat Cells, 5c.c7 Primary Mouse T Cells and Fura-2

The prototypical cell line to study T cell signalling is the Jurkat cell line.[morgan2023] It was obtained from the blood of a boy with T cell leukaemia.[schneider1977] Different

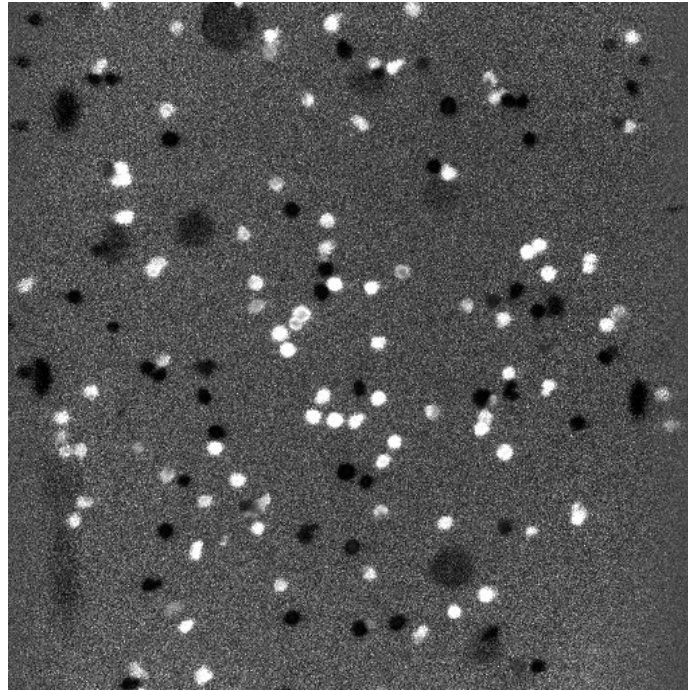


Figure 4.1.: Single frame showing the ratio of the 340nm and 380nm images from a recording of human Jurkat cells. Activated cells appear lighter, unactivated cells darker than the background. Big dark circles are out of focus cells that have not yet settled on to the plate.

cell lines within the Jurkat family are described by Abraham and Weiss.[[abraham2004](#)] They provide a timeline of discoveries linked to Jurkat cells and t cell receptor signalling. Another type of t cells used in signalling studies are gathered from mice.

In order to be able to measure the intracellular  $\text{Ca}^{2+}$  concentration of cells they can be labelled with Fura-2. This method provides a way to record the  $\text{Ca}^{2+}$  concentration of multiple cells over a time period.[[martinez2017](#)] Challenges encountered when using Fura-2 on certain cell types are described by Roe, Lemasters and Herman along with their respective solutions.[[roe1990](#)]

### 4.3. Measuring the Calcium Concentration of T Cells

After the cells have been labelled with Fura-2, a recording of up to 15 to 20 minute can be generated. To achieve this the cells and stimulant are photographed at both 340nm and 380nm wavelength once per second. The resolution of the images are 1.6 $\mu\text{m}$  per pixel. By calculating the ratio of the two images at each pixel the  $\text{Ca}^{2+}$  concentration can be observed. An exemplary resulting image showing the ratio is shown in figure 4.1. The t cells appear a lighter shade than the background when activated and darker when not activated.

To activate the cells in the duration of the recording they are transferred to a plate



covered with replicas of the MHC-peptide complex normally present on APCs. This plate is then recorded as described above. For a negative control the plate is not covered with peptides, while for the positive control the peptide covering on the plate is very dense. Recordings of different densities in peptides lead to activation of a percentage of t cells.

## **4.4. Processing the Data**

To track single t cells moving around during the video the sum of the 340nm and 380nm image of each second is calculated. This image provides the basis for separating t cells from the background. On this image all t cells will appear similarly light in colour. Therefore, it is used to track the movement of cells. Each cell is numbered, such that the same cell will have the same number during the video. For some cells the trajectory tracking is not perfect, resulting in a split of the numbering into multiple numbers for the same cell. The position and shade during both 340nm and 380nm as well as the ratio of each particle and each frame is then recorded into the data structure used in this work. The first roughly 50 frames at the start of the recording are discarded due to the video being out of focus. Additionally, cells only appearing in fewer than 300 frames are discarded as they most likely represent trajectories incorrectly tracked or split. The resulting data is then stored in a matrix structured as described in table [4.1](#).



## 5. Approximating the Calcium Concentration

If we have a look at the typical trajectory of the calcium concentration in activated and unactivated cells, shown in figure 5.1, we can see differences emerging. For one the maximum concentration value reached by most activated cells is higher. Another distinguishing feature is the presence of a steep incline at the moment of activation.

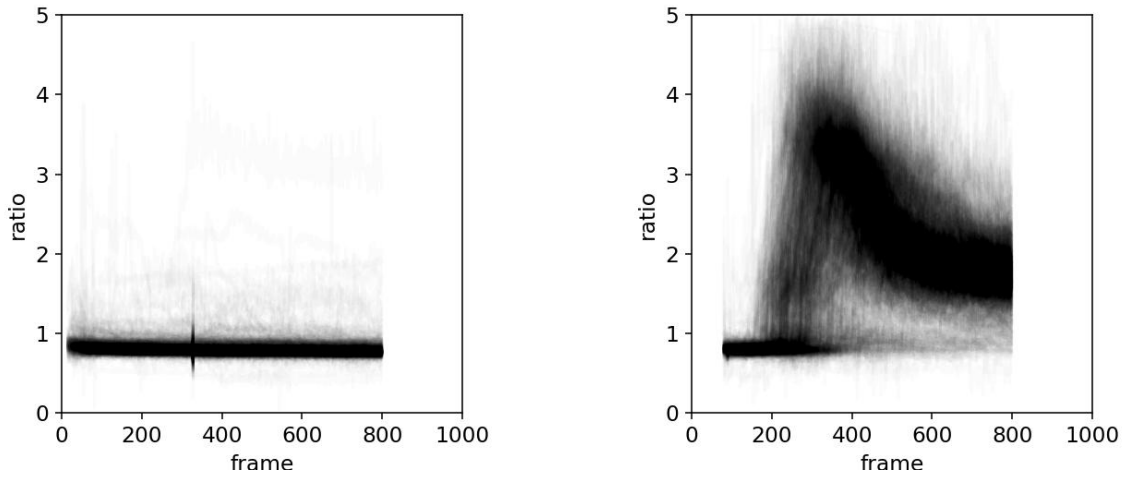


Figure 5.1.: Two plots of the overlapping calcium concentration time series of cells. On the left a negative control and on the right a positive control of mouse cells.

By modelling the time series with a function incorporating features such as the increase, maximum value and oscillations present in the decrease afterwards, we can extract these features more easily. By doing this, using approximation methods from chapter 2, we hope to have an easier method to answer the questions from the introduction.

### 5.1. Approximation Function

From studying the data in the two control groups we find to expect a function close to

$$f_{unac}(x) := u \quad (5.1)$$

for unactivated cells and

$$f_{ac}(x) := \begin{cases} \frac{a-u}{1+e^{-k_1(x-w_1)}} + u & \text{if } x \leq t \\ \frac{a-d}{1+e^{-k_2(x-w_2)}} + d & \text{else} \end{cases} \quad (5.2)$$

## 5. Approximating the Calcium Concentration

---

$u$ ...	average value before activation,
$a$ ...	value reached at the peak of activation,
$d$ ...	average value after activation,
$k_1$ ...	steepness of increase,
$k_2$ ...	steepness of decrease,
$w_1$ ...	time point at which the increase happens,
$w_2$ ...	time point at which the decrease happens,
$t$ ...	time point at which the increase ends, and the decrease starts,

Table 5.1.: List of parameters and their interpretation.

for activated cells. The parameters can be understood as described in table 5.1.

Figure 5.2 shows the above functions 5.1 and 5.2, and shows the relations to the parameters in unactivated and activated cells. The similarity between these functions and figure 5.1 can be observed.

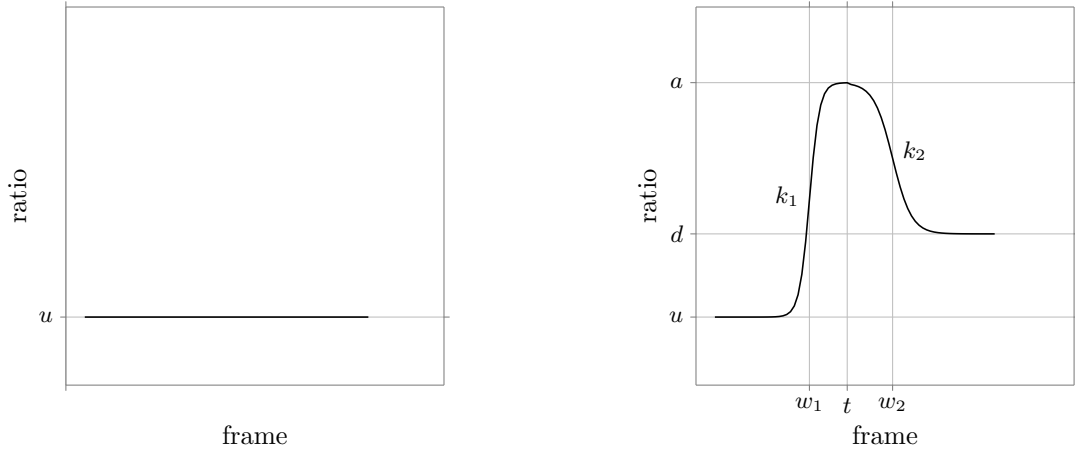


Figure 5.2.: Left shows the function  $f_{unac}$  defined in 5.1 with the parameter  $u$ . The right shows the function  $f_{ac}$  defined in 5.2 with the parameters  $u, d, a, w_1, t, w_2, k_1$  and  $k_2$ .

For our model to make sense we have to impose some conditions onto the parameters. We expect

$$0 \leq u \leq d \leq a, \quad w_1 \leq t \leq w_2, \quad k_1 > 0 \quad \text{and} \quad k_2 < 0.$$

There are multiple ways in which the parameters of  $f_{ac}$  can be chosen to get a function similar to  $f_{unac}$ . If  $w_1$  is very large or  $u \approx d \approx a$  then  $f_{ac}$  approaches a constant value of  $u$ , thus approximating  $f_{unac}$ . If the approximation of a cell has parameters with  $w_1$  very large or  $u \approx d \approx a$  we can therefore expect it to be of an unactivated cell. Otherwise, it is more probable to be activated.

## 5.2. Implementation of the Approximation

Now that we have defined our model functions we will implement a routine that fits such a  $f_{ac}$ -function through the data points of a particle recording.

First we give the pseudocode for approximating a single particles time series with the approximation function described above. It takes a (frame, ratio)-matrix of a single particle as input and returns the corresponding parameter list of the approximation.

---

**Algorithm 4:** Approximate

---

```

input  : particle data as (frame, ratio) matrix
output: parameters describing the approximation

1 begin
2   set boundaries for parameters
3   set start values for parameters
4   use Trust Region Reflective Algorithm with boundaries and start values to get
   parameters
5   calculate corresponding approximation and add as fit_sigmoid columns to data
   matrix
6   return parameters
7 end

```

---

The parameters of  $f_{ac}$  used in the approximation are not independent of each other as we want to choose  $t$  to be the point at which the increasing part of the function,  $(a - u)/(1 + e^{-k_1(x-w_1)})$ , almost reaches the value  $a$ . We choose

$$t := w_1 - \log(1/0.99 - 1)/k_1 = w_1 - \log(1/99)/k_1$$

as the function has had 99% of the increase of the sigmoid curve up to this point.

Setting the boundaries in line 2 is non-trivial. We have noted that a condition such as  $0 \leq u \leq d \leq a$ ,  $w_1 \leq t \leq w_2$ ,  $k_1 > 0$  and  $k_2 < 0$  are expected. We want to impose them using boundaries in which the parameters must lie. However, boundaries for each parameter must not depend on other parameters. We can circumvent this by changing the parameters to be relative to each other. As  $u \leq d \leq a$  we choose to use the three parameters  $u$ ,  $d - u$  and  $a - d$ . We can then set the lower boundary to be 0 which ensures

$$\begin{aligned}
0 \leq u \quad \wedge \quad 0 \leq d - u \implies d \geq u \quad \wedge \quad 0 \leq a - d \implies a \geq d \\
\implies 0 \leq u \leq d \leq a.
\end{aligned}$$

Using the same method, we choose the parameters  $w_1 - start$  and  $w_2 - w_1$ , where *start* is the first frame in which the particle was tracked. The resulting boundaries are described in table 5.2, where we set min val, max val and median val as the minimum, maximum and median of the particles' ratio data respectively while start and end is the first and last frame where data was recorded for this particle.

## 5. Approximating the Calcium Concentration

---

The condition  $t \leq w_2$  can be violated, but it is ensured that at least  $w_1 \leq w_2$ .

The other conditions are met as  $k_1 \in [0.05, 10] \implies k_1 > 0$  while  $k_2 \in [-1, -0.01] \implies k_2 < 0$  and

$$t = w_1 - \underbrace{\log(1/99)/k_1}_{<0} \geq w_1.$$

parameter	lower bound	upper bound	starting value
$u$	min val	max val	min val
$d - u$	0	max val	median val - min val
$a - d$	0	max val	max val - median val
$w_1 - start$	0	end - start	0
$w_2 - w_1$	0	end - start	(end - start) / 2
$k_1$	0.05	10	0.1
$k_2$	-1	-0.01	-0.03
$d$	min val	2 max val	median val
$a$	min val	3 max val	max val
$w_1$	start	end	start
$w_2$	start	2 end - 2 start	(start + end)/2

Table 5.2.: Upper and lower bounds as well as starting value for each of the parameters. The boundaries and starting values of  $d, a, w_1$  and  $w_2$  are derived from the parameters used in the implementation of the approximation, shown above the double line.

Starting values can have a big impact on the approximation reached by the algorithm. We want to choose starting values close to the expected resulting parameters. By choosing the starting value of  $w_1 - start$  as 0, which corresponds to choosing  $w_1 = start$ , we favour the first increase in the data to be the point of activation. Otherwise, we are more likely to mistake an oscillation later in the data as the activation point. As we do not know when the activation happens when setting the boundaries we guess that  $w_2$  will lie somewhere in the middle. Therefore we choose  $(end - start)/2$  as the starting value for  $w_2 - w_1$ . The other starting values are chosen as we expect  $u$  to be low,  $a$  to be high,  $d$  to lie somewhere in the middle. Experimenting showed that  $k_1$  often has a value around 0.1 while  $k_2$  lies around  $-0.03$ .

Using algorithm 4 we now describe a routine which handles reading the data, some necessary preprocessing steps and saving of the resulting parameter lists.

---

**Algorithm 5:** Approximation Loop

---

**input** : file containing data matrix as described in section 4.1  
**output**: parameters of the approximation of all particles as a matrix

```
1 begin
2   read data
3   filter data
4   for each single particle do
5     particle data := (frame, ratio) columns of this particle
6     if length of particle data is too short then
7       | skip
8     end
9     parameters := approximate(particle data)
10    optionally show ratio data and approximation
11    save parameters
12  end
13  return matrix of all parameters
14 end
```

---

Filtering the data is necessary as the ratio can be very large if the denominator is small. Values are therefore bounded to lie within the interval  $[0, 5]$ . Any values higher than 5 are almost certainly caused by measurement errors. Values below 0 are definitely incorrect, as both the denominator and numerator are measured as the brightness of a pixel, which can not be negative.

The visualization in line 10 of algorithm 5 generates images such as figure 5.3.

This work uses the python scipy function `scipy.optimize.curve_fit(function, xdata, ydata, p0=starting_values, method='trf', bounds=(lower_bounds, upper_bounds))` as it provides all the necessary functionality. The method parameter `trf` stands for Trust Region Reflective, as described in section 2.2.3.

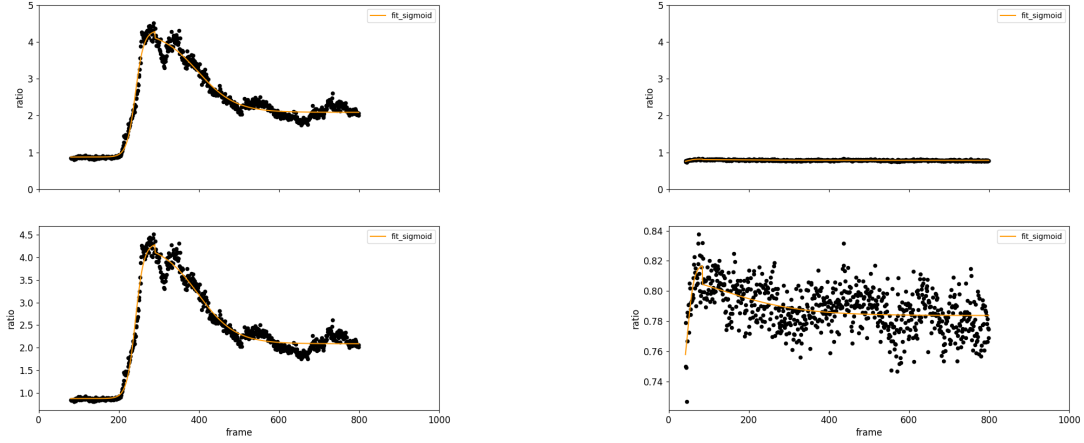


Figure 5.3.: The left plot shows the data in black and approximation in orange of an activated cell. The first plot is scaled from 0 to 5, the second one is scaled to fit the data. The right plot shows the same of an unactivated cell.

### 5.3. Analysis of the Approximation

We now give data on the parameters found from the above approximation. Some statistics are found in table 5.3. Figure 5.4 shows the distribution of the resulting parameters of the approximation. From the figure it seems the differences between activated and unactivated cells is biggest in the parameters activated value  $a$ , decreased value  $d$  as well as the steepness of increase  $k_1$ .

As the datasets are not perfectly labelled, meaning there are activated cells in the negative control and vice versa, we have relatively high standard deviation.

We can use the mean and standard deviation of each of the parameters to find data points that can be considered outliers. We expect wrongly-labelled data, e.g. activated cells in the negative control, to be an outlier in the parameters  $a$  and  $d$ . However, activated cells in the positive control might have a decreased value  $d$  that is very low, around  $u$ . This makes it difficult to distinguish activated from unactivated cells when looking at the parameter  $d$ . Therefore, we choose  $a$  as the only parameter when filtering for these kinds of outliers.

A particle from the positive control dataset that has a value in parameter  $a$  higher than the median should still be classified as activated. Only a value lower than some threshold indicates an unactivated cell. The same holds for values of  $a$  lower than the median in the negative control dataset. In short, we want to filter out particles with a high value of  $a$  in the negative control and those with a low value of  $a$  in the positive control dataset. Therefore, the threshold has to be specified as a lower and upper bound in multiples of the standard deviation.

We give pseudocode for the detection of outliers.



		Positive Control		Negative Control		
	Parameter	Average	Standard Deviation	Average	Standard Deviation	Difference
human cells	$a$	2.808	0.461	0.923	0.669	1.885
	$u$	0.663	0.521	0.613	0.311	0.05
	$d$	1.937	0.491	0.685	0.412	1.252
	$k_1$	0.263	0.428	0.524	0.963	-0.261
	$k_2$	-0.059	0.164	-0.163	0.292	0.104
	$w_1$	142.228	124.012	171.062	131.563	-28.834
	$w_2$	445.386	185.971	478.843	190.792	-33.457
mouse cells	$a$	2.9	0.907	0.876	0.186	2.024
	$u$	0.889	0.27	0.79	0.093	0.099
	$d$	1.749	0.407	0.804	0.129	0.945
	$k_1$	0.15	0.409	1.161	1.235	-1.011
	$k_2$	-0.1	0.195	-0.133	0.267	0.033
	$w_1$	295.809	77.207	100.712	112.352	195.097
	$w_2$	469.952	105.375	304.283	179.834	165.669

Table 5.3.: Statistics of the parameters retrieved from approximating the human cell data.

**Algorithm 6:** Find Outliers

---

**input** : data as matrix of all particle parameters of the approximation, threshold  
as pair, parameters\_used as list  
**output**: set of indices of the outliers

```

1 begin
2   outliers := empty set
3   for parameter in parameters_used do
4     mean := mean(data[parameter])
5     std := standard_deviation(data[parameter])
6     interval := [mean - std · threshold[0], mean + std · threshold[1]]
7     outliers = outliers ∪ {data[index] : data[parameter] ∉ interval}
8   end
9   return outliers
10 end

```

---

The question of how to choose the threshold will be discussed next. As we do not have information on what percentage of cells behaved correctly in the positive and negative control we do not have enough information to choose threshold values without guessing. Instead, we can manipulate the threshold as a multiple of the standard deviation until we filter out incorrectly labelled data, but would filter out correctly labelled data points if we increase the value. This trial and error approach led to different values for each of the four control datasets, which can be seen in table 5.4.

Naturally we can use the same outlier detection with different parameters to find particles

## 5. Approximating the Calcium Concentration

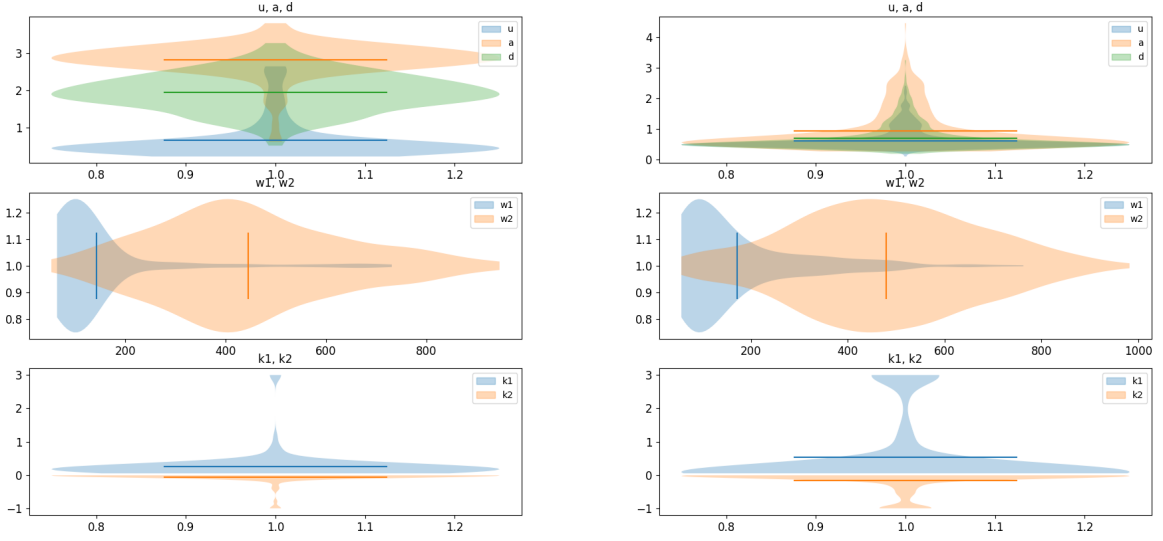


Figure 5.4.: Violin plots of parameters  $u, a, d, w_1, w_2, k_1$  and  $k_2$  from the approximations. The parameters of the positive control are on the left and those of the negative control are on the right. Both are of human cells.

dataset	lower bound	upper bound
human positive	mean $-3$ std = 1.582	$\infty$
human negative	$-\infty$	mean $+0.5$ std = 1.306
mouse positive	mean $-2$ std = 1.41	$\infty$
mouse negative	$-\infty$	mean $+3$ std = 1.445

Table 5.4.: Thresholds in outlier detection in the different datasets.

where the approximation failed to yield a good result.

These results will be used in section 7.1 to remove wrongly-labelled data from the datasets.

### 5.4. Adding Oscillation in the Decrease

In order to answer the questions from chapter 1 concerned with the oscillations happening in the decrease of the  $\text{Ca}^{2+}$  concentration we want to model them as well. We use a method often used when analysing oscillating data, called Fourier Transformation.

Fourier Transformation is used when an application is concerned with cyclic temporal data. Examples are sound waves, seismic data or oscillations of a skyscraper in strong wind. This data can be represented as a function of amplitude over time. Most of the time we are not interested in the amplitude at a specific point in time, as a temporal shift would represent very similar information. Such a shift is demonstrated in figure 5.5.

As the function of sound waves or oscillations in the  $\text{Ca}^{2+}$  concentration in t cells is almost cyclic we might be interested in a decomposition into simple cyclic function, such as sine. We can then analyse the most prominent frequencies and their respective amplitudes.

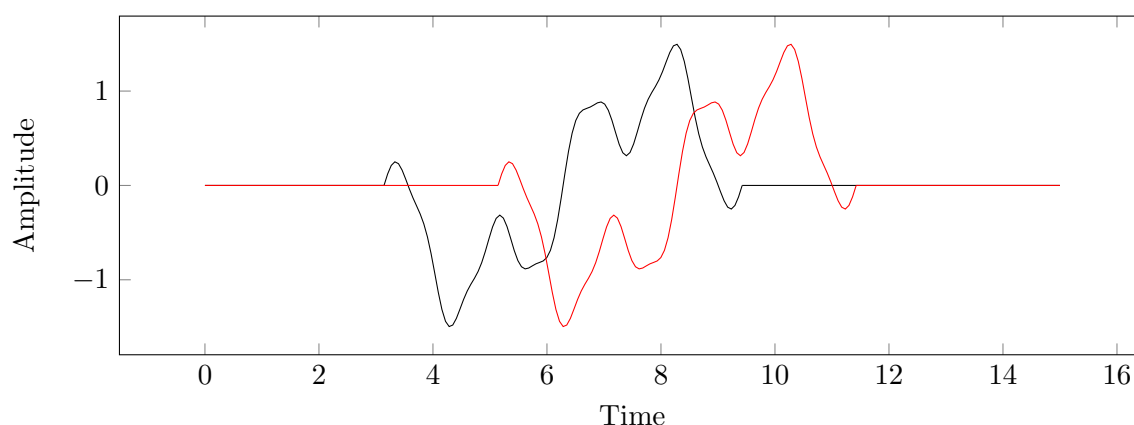


Figure 5.5.: Two signals that differ by a temporal shift.

This gives a representation of the data, that can be easier to interpret. Fast Fourier Transformation (FFT) is an algorithm that transforms temporal data into such a representation of a weighted sum of sines.

As the oscillations happen in the decrease of the  $\text{Ca}^{2+}$  concentration we apply FFT to that part of the data. We can then filter out the 10 frequencies with the highest amplitudes and use them to further analyse the oscillations. This gives an even better approximation of the data, which can be seen in figure 5.6.

We can store the data gathered using the FFT as a list of frequencies and corresponding amplitudes.

[TODO analyse frequencies and amplitudes]

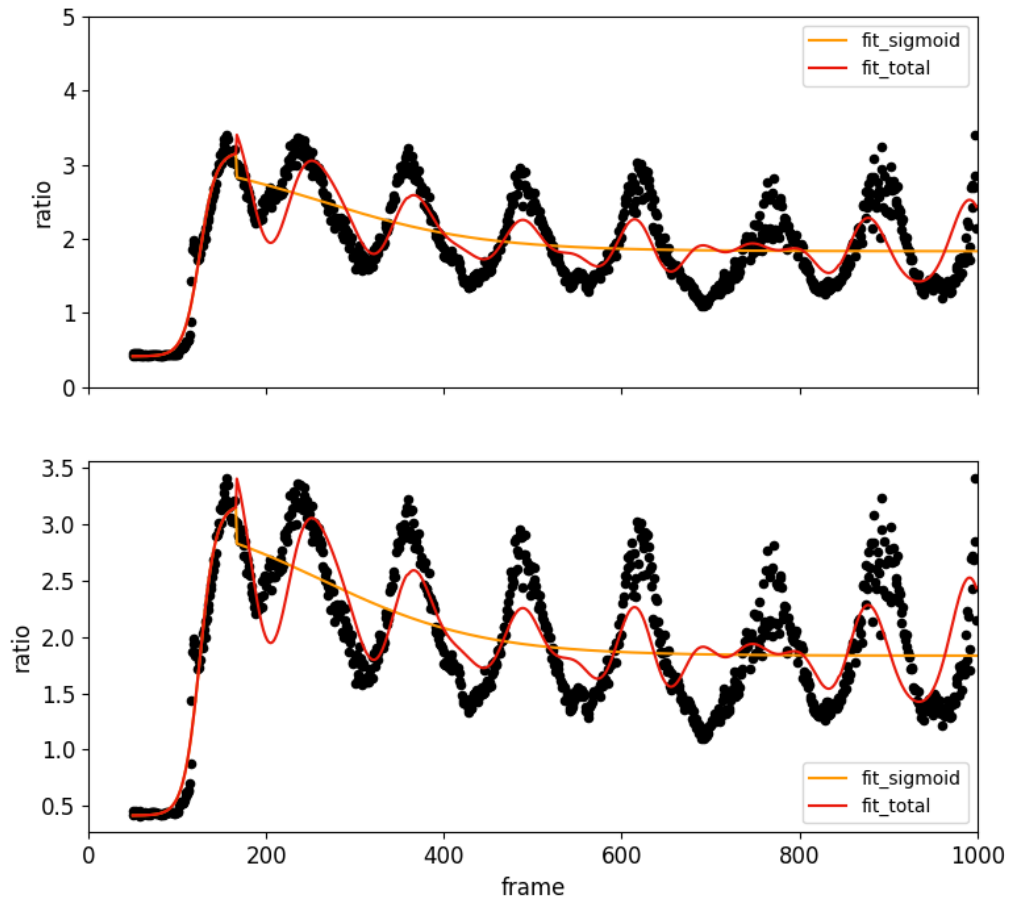


Figure 5.6.: The data of an activated cell with heavy oscillation is shown in black, simple approximation in orange and the approximation with FFT added in red. The first plot is scaled from 0 to 5, the second one is scaled to fit the data.

## 6. Clustering Algorithm and Application

The objective of classification is to find assignments between data points and categories. For some applications this can be done by taking correctly labelled data and comparing a new data point to the data points in different categories to see which category best fits. One such algorithm is k-nearest-neighbour. In our context the issue with this approach is that the data is only labelled as to which experiment it came from, e.g. positive control in human cells, negative control in mouse cells. However, as noted before not all cells from these experiments behaved as we expected them to, e.g. some cells activated in the negative control or did not activate in the positive control. Therefore, we choose to use a clustering algorithm which does not have the need for classified training data.

### 6.1. Gaussian Mixture Model

This section follows the article Gaussian Mixture Model by Reynolds [reynolds2009].

Often gathered observations are distributed as a normal distribution. These distributions have a density function

$$g(x|\mu, \Sigma) = \frac{1}{(2\pi)^{D/2}|\Sigma|^{1/2}} \exp\left(-\frac{1}{2}(x - \mu)^T \Sigma^{-1}(x - \mu)\right)$$

with parameters  $D$  called the dimension,  $\mu$  called the mean vector and  $\Sigma$  called the covariance matrix.

As we are concerned with clustering data points we expect the observed data points from different clusters to have different parameters in the normal distribution they come from. Assuming we have  $n$  different data sources gives us normal distributions  $g_i(x|\mu_i, \Sigma_i)$  where  $i = 1, \dots, n$ . Additionally, we might have more data points being generated from some normal distributions while less from others. We can express this using another weight parameter  $w_i$  with  $i = 1, \dots, n$ . To normalize the weights we set the constraint  $\sum w_i = 1$ .

The distribution describing the entire dataset now can be described with the distribution

$$p(x) = \sum_{i=1}^n w_i g(x|\mu_i, \Sigma_i). \quad (6.1)$$

Gaussian Mixture Model is a method to retrieve these parameters  $w_i$ ,  $\mu_i$  and  $\Sigma_i$  for some  $D$  dimensional data points generated from  $n$  normal distributions.

From these parameters it is easy to cluster the data as we know where data points from the different clusters are expected to lie.

From equation 6.1 we expect every  $\Sigma_i$  to be independent of each other. In the context of Gaussian Mixture Models this is called having a full covariance matrix. However, we can eliminate some of the variables in the covariance matrix if we choose a diagonal covariance

matrix. Additionally, we might specify to use the same covariance matrix for all  $i$ , which is called tied in this context.

Choosing a full covariance matrix is not necessary even if the data is expected to have statistically independent features, as the overall density is compromised from multiple normal distributions with diagonal  $\Sigma_i$ . This enables us to model correlations between features.

The question now is how we can derive the parameters  $w_i, \mu_i$  and  $\Sigma_i$ . We choose the approach which chooses the parameters where the likelihood that the data was generated by these parameters is maximal. This is known as maximum likelihood estimation. The likelihood can be expressed as

$$L(w_i, \mu_i, \Sigma_i | X) = p(X | w_i, \mu_i, \Sigma_i) = \prod_{t=1}^n p(x_t | w_i, \mu_i, \Sigma_i)$$

with  $X = (x_1, \dots, x_n)$  being the recorded data. As  $L(w_i, \mu_i, \Sigma_i | X)$  is non-linear in the parameters deriving the maximum is not trivial. Instead, we use an iterative approach which approaches the solution. Define  $\lambda = (w_i, \mu_i, \Sigma_i)$ . Simplifying to a diagonal covariance matrix gives us the iterative algorithm where we define the successor values  $\bar{\cdot}$  as

$$\begin{aligned} Pr(i | x_t, \lambda) &:= \frac{w_i g(x_t | \mu_i, \Sigma_i)}{\sum_{k=1}^n w_k g(x_t | \mu_k, \Sigma_k)} \\ \bar{w}_i &:= \frac{1}{n} \sum_{t=1}^n Pr(i | x_t, \lambda) \\ \bar{\mu}_i &:= \frac{\sum_{t=1}^n Pr(i | x_t, \lambda) x_t}{\sum_{t=1}^n Pr(i | x_t, \lambda)} \\ \bar{\sigma}_i^2 &:= \frac{\sum_{t=1}^n Pr(i | x_t, \lambda) x_t^2}{\sum_{t=1}^n Pr(i | x_t, \lambda)} - \bar{\mu}_i^2. \end{aligned}$$

for  $w_i, \mu_i$  and  $\sigma_i^2$  respectively. One can show that with this iteration rule we have  $p(X | \bar{\lambda}) \geq p(X | \lambda)$ . The value  $Pr(i | x_t, \lambda)$  is known as the a posteriori probability for the  $i$ -th component.

From the parameters  $w_i, \mu_i$  and  $\sigma_i^2$  we can get the probability of a data point belonging to the  $i$ -th cluster. This data point can be either one of the ones used to get the parameters or a new one.

## 6.2. KMeans

We want to explore a second clustering algorithm. Like Gaussian Mixture Model this method assigns data points to clusters after having been trained with unlabelled data.

Once again we assume to have  $k$  different data sources from where the data stems. As the data from every of these resulting clusters will be close to each other, we have that the variance within the cluster is relatively small compared to the variance of data points from different clusters.

The variance of data points  $(x_n)_{n=1,\dots,m}$  is calculated as

$$\text{Var}((x_n)_{n=1,\dots,m}) = \frac{1}{m} \sum_{n=1}^m \|x_n - \mu\|^2, \quad \text{where} \quad \mu = \frac{1}{m} \sum_{n=1}^m x_n.$$

We can therefore formulate the problem as a minimization problem. Using  $k$  clusters  $S_1, \dots, S_k$ , with  $|S_l|$  data points in each, we want to minimize the sum of variants

$$\sum_{l=1}^k \sum_{x \in S_l} \|x - \mu_l\|^2 = \sum_{l=1}^k |S_l| \text{Var}(S_l).$$

We want to show that this is equivalent to minimizing

$$\sum_{l=1}^k \frac{1}{|S_l|} \sum_{x,y \in S_l} \|x - y\|^2.$$

This follows from the equality

$$\begin{aligned} & \frac{1}{|S_l|} \sum_{x,y \in S_l} \|x - y\|^2 = \\ & \frac{1}{|S_l|} \sum_{x,y \in S_l} (\|x\|^2 - 2\|x\| \cdot \|y\| + \|y\|^2) = \\ & \frac{1}{|S_l|} (|S_l| \sum_{x \in S_l} \|x\|^2 - 2 \sum_{x,y \in S_l} \|x\| \|y\| + |S_l| \sum_{y \in S_l} \|y\|^2) = \\ & \frac{1}{|S_l|} (|S_l|^2 E(S_l^2) - 2(\sum_{x \in S_l} \|x\|)(\sum_{y \in S_l} \|y\|) + |S_l|^2 E(S_l^2)) = \\ & 2|S_l| E(S_l^2) - 2|S_l| E(S_l)^2 = \\ & 2|S_l| \text{Var}(S_l). \end{aligned}$$

Minimizing is hard, but is typically solved by the approximation using the following algorithm consisting of two steps.

- Assign all data points to clusters  $S_1, \dots, S_k$ , by choosing the cluster  $S_l$  with the closest mean  $\mu_l$ .
- Update the means  $\mu_l$  by calculating them as the mean of the data points assigned to  $S_l$ .

We formulate this mathematically as the successor  $\hat{S}_l$  and  $\hat{\mu}_l$  of  $S_l$  and  $\mu_l$  respectively being

$$\hat{S}_l := \{x : \|x - \mu_l\| \leq \|x - \mu_j\| \forall j \in \{1, \dots, k\}\} \quad \hat{\mu}_l := \frac{1}{|\hat{S}_l|} \sum_{x \in \hat{S}_l} x.$$

From the definition of  $\hat{S}_l$  and  $\hat{\mu}_i$  it follows that

$$\sum_{l=1}^k \frac{1}{|\hat{S}_l|} \sum_{x,y \in \hat{S}_l} \|x - y\|^2 \leq \sum_{l=1}^k \frac{1}{|S_l|} \sum_{x,y \in S_l} \|x - y\|^2.$$

The convergence of the algorithm towards a minimum seems likely. The choice of initial values can have a big impact on the result.

### 6.3. Implementation of the Clustering Algorithm

Python offers an implementation of Gaussian Mixture Model and KMeans with the sklearn package. The function with parameters relevant to us is

`sklearn.mixture.GaussianMixture(n_components, covariance_type, n_init)` and `sklearn.cluster.KMeans(n_clusters, n_init)`. The number of components `n_components` or `n_clusters` can be any positive integer. The `covariance_type` can be one of 'full', 'tied', 'diag' or 'spherical' and describes what type of covariance matrix is used. The parameter `n_init` lets the algorithm run multiple times and returns the parameters of the best clustering achieved.

As the input of the clustering we use data points of the form `[a, u, d, k1, k2, w1, w2]`, where `a, u, ..., w2` are the parameters of the approximation from chapter 5. As our goal is to separate data points from the four data sets mouse cells and human cells each with a negative and a positive control, we use all particles as input. The pseudo code below describes the steps performed to reach a clustering of the data.

---

**Algorithm 7:** Separate

---

**input** : parameters of the approximations of all particles in all data sets  
**output:** assignments to different clusters for each particle, parameters specifying each cluster

```

1 begin
2   initialize Gaussian Mixture or KMeans by specifying the number of
     components and covariance_type for Gaussian Mixture
3   apply clustering method to matrix of all parameters of the approximations of
     all particle data sets
4   assign particles to clusters according to clustering results
5   compare assignments from clustering to those of the data set the data stems
     from
6   return assignments to clusters, parameters specifying every cluster
7 end

```

---

When comparing different covariance types in the Gaussian Mixture we see that using 'diag' we have the lowest error rate. The details are shown in table 6.1. Why reducing the number of parameters in the covariance matrix can yield better results is described in section 6.1.



full: 13.23%	tied: 12.7%
diag: 7.17%	spherical: 31.52%

Table 6.1.: Error as a percentage of particles being assigned the wrong component.

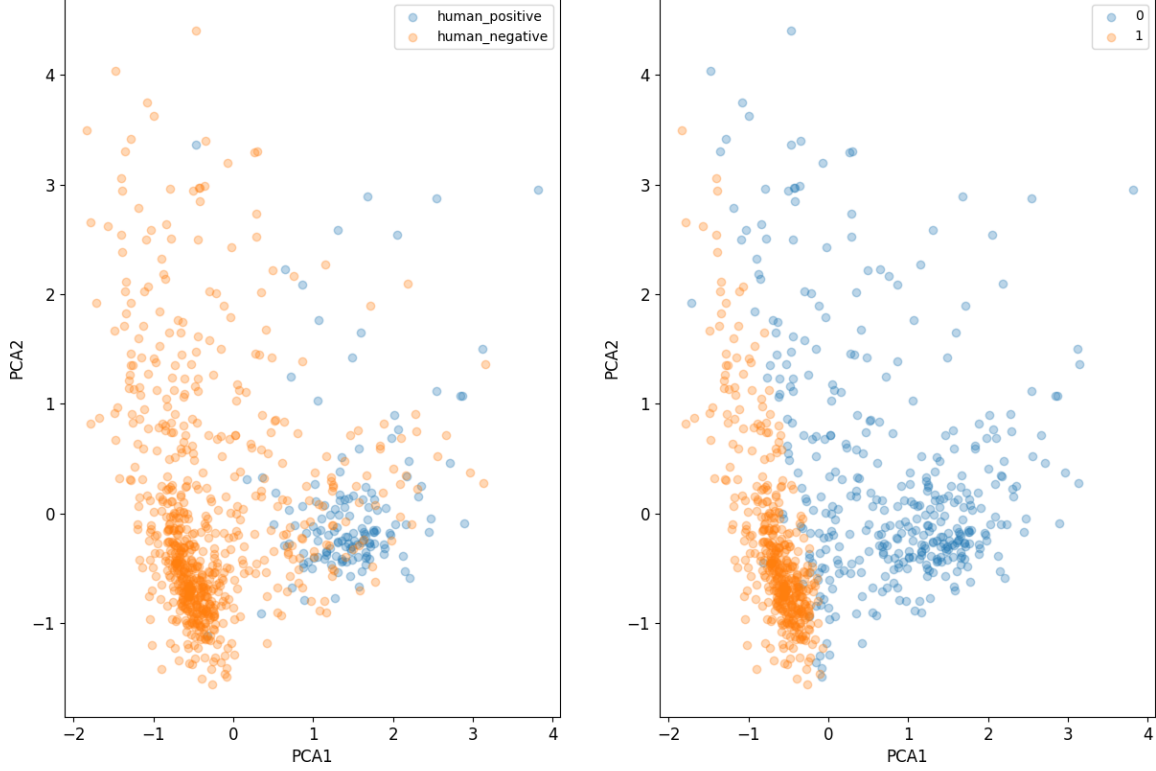


Figure 6.1.: Visualization of the clustered data points. The left image depicts the clustering according to positive and negative control on humans t cells. The right image shows the clustering according to Gaussian Mixture.

Using a diagonal covariance matrix we can now try to separate the data sets and visualize the results. As the data is 7 dimensional we show lower dimensional representations of the data both as it is assigned according to the data set it stems from as well as the assignment from algorithm 7.

Choosing good axis for visualizing high dimensional data is tricky. One approach for minimizing the data lost by the lower dimensional representation is called Principal Component Analysis. Axis are specifically chosen to maximize variance along those axes, which we assume corresponds to information displayed along the axis. The drawback is that the new axis can be more difficult to intuitively understand. The results can be seen in figure 6.1, figure 6.2, figure 6.3 and 6.4.

By comparing which data points are from which data set and where they were assigned by the clustering method we can find an assignment between the two.

The relevant information derived from the Gaussian Mixture clustering is the means and

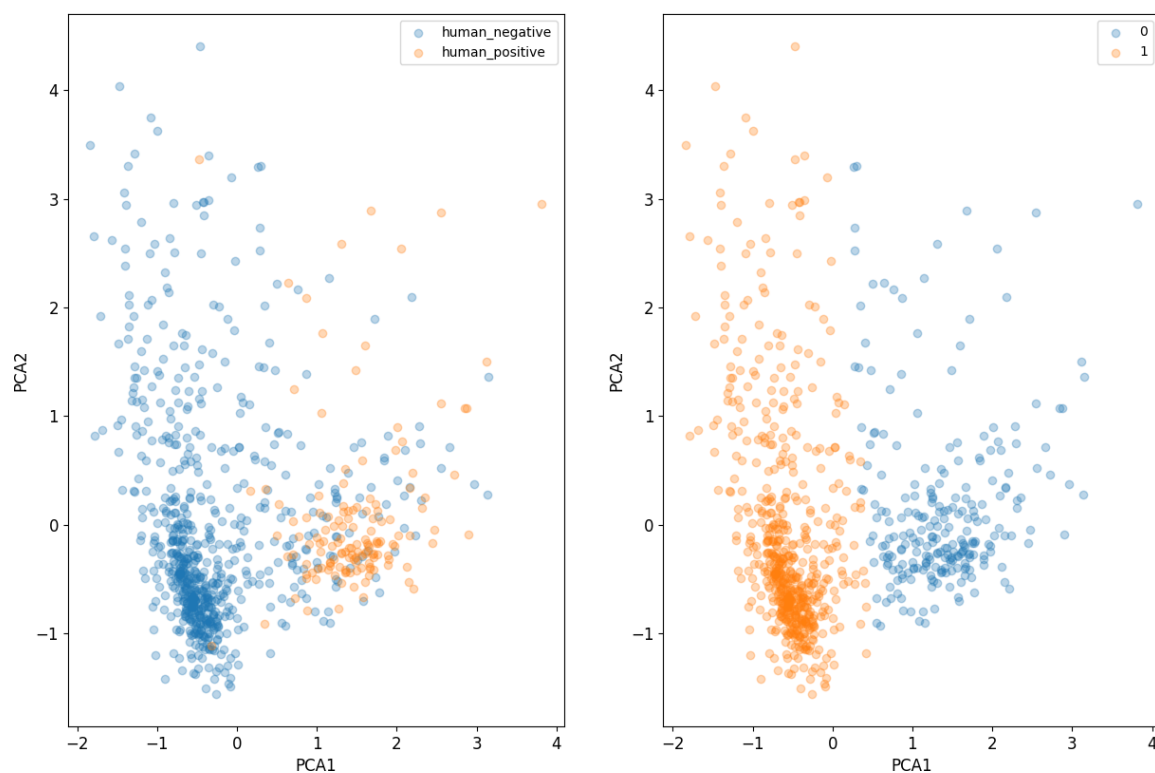


Figure 6.2.: Visualization of the clustered data points. The left image depicts the clustering according to positive and negative control on humans t cells. The right image shows the clustering according to KMeans.

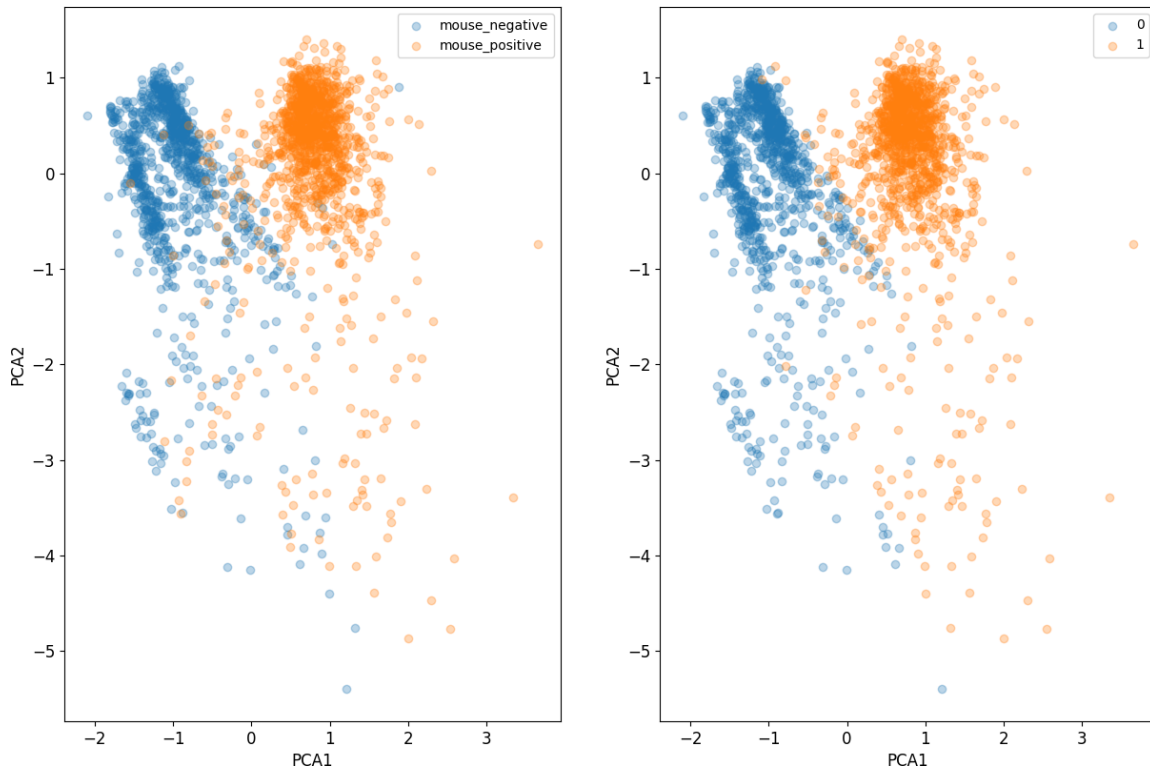


Figure 6.3.: Visualization of the clustered data points. The left image depicts the clustering according to positive and negative control on mouse t cells. The right image shows the clustering according to Gaussian Mixture.

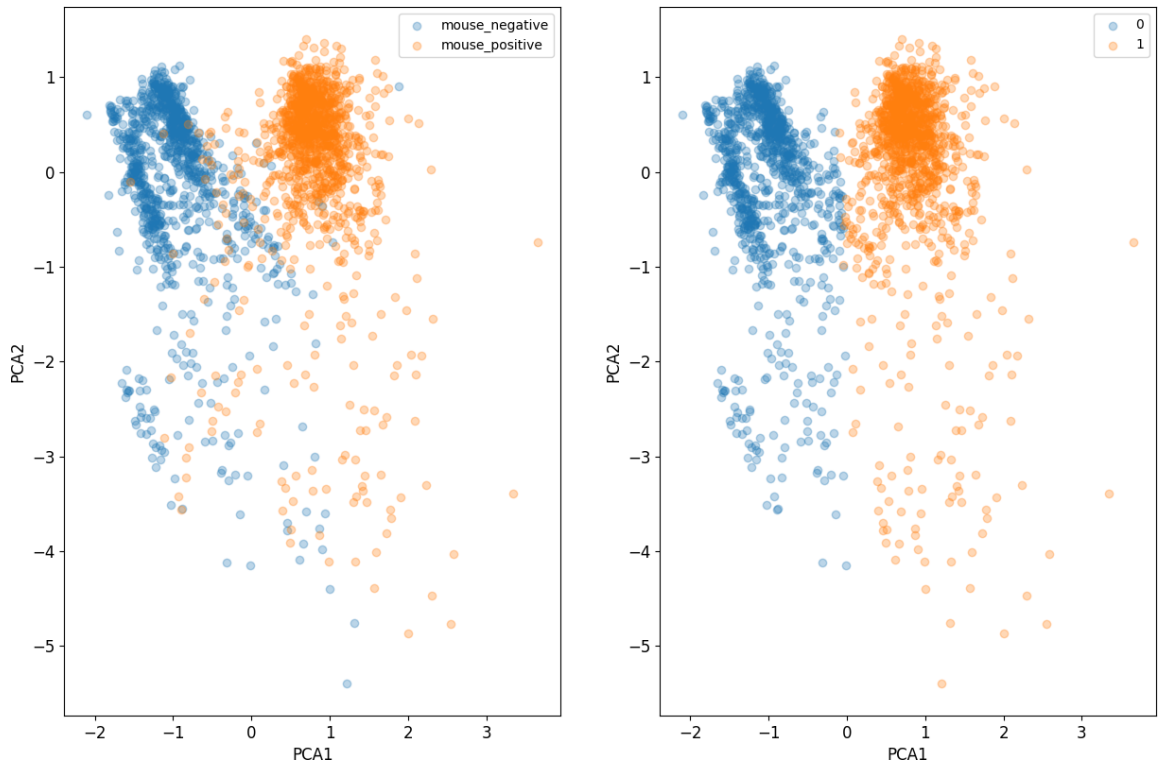


Figure 6.4.: Visualization of the clustered data points. The left image depicts the clustering according to positive and negative control on mouse t cells. The right image shows the clustering according to KMeans.

covariances of the four components. For KMeans clustering the means of the components are relevant. In both cases we can decide which cluster a new data point belongs to from this information. A use case might be to find percentages of activated cells in an experiment. Distinguishing between mouse and human cells does not have a clear use case. When specifying `n_components=2` we assume to have a cluster for activated and a second for unactivated cells.

In comparison, to the approach focusing on outlier detection in section 5.3 we now have an approach that is not only not dependent on parameters specified by a user, but can also be applied to a greater set of problems. A proposed way of answering the research questions from chapter 1 using these methods is described in chapter 7.



## 7. Results

This chapter gives answers to the questions from chapter 1. To answer the methods described in this work, such as approximation, clustering and outlier detection, are combined and used.

### 7.1. Proposed algorithm for Detecting Activated T Cells

The first and most relevant question was "Which criteria can distinguish between unactivated, activated and pre-activated cells?".

First we give a method for filtering the pre-activated cells from a dataset. From their nature we expect a high value in  $\text{Ca}^{2+}$  concentration at the start of the recording. Using the approximation from chapter 5 it is easy to get the approximate  $\text{Ca}^{2+}$  concentration value at the start of the recording, as it is the parameter  $u$ . Using the algorithm 6 with parameters threshold as  $[\infty, 0.5]$  and parameters\_used as  $[u]$  gives good results. It returns the indices of particles, which are pre-activated in the data sets of the positive controls.

After having filtered out pre-activated particles, we want to distinguish between unactivated and activated particles. For this we propose the following steps:

1. get positive control, negative control and experiment recordings
2. transform each particle time series of all three data sets to the parameter list by approximating it with a combination of sigmoid functions, according to chapter 5, using the algorithm 5
3. use outlier detection, which is described in algorithm 6, to filter out non-conforming cells from both the positive and negative control, as well as pre-activated cells, and particles where the approximation yielded suboptimal results
4. use clustering method, as one described in chapter 6, with parameters of filtered negative and positive control as input to get the clustering parameters
5. predict the membership of the experiment particle parameters to the clusters to get a prediction of activation

This algorithm is implemented in Python and shown in appendix A.

[TODO results of applying it to experiment data]

The algorithm can be adapted by using different clustering methods, or specifying other methods of separating the particles based on the parameters derived.

## 7.2. Types of Activated Cells

Question: Do different types of activated cells exist? How are they different?

Answer: Apply Gaussian Mixture Clustering to activated cells only. (Separate human and mouse cells, otherwise two clusters of each)

## 7.3. Oscillation in Decrease

Question: With which frequencies does the Calcium concentration repeat after activation?

Answer: Results from frequency analysis

## 7.4. Difference between Mouse and Human Cells

Question: Is there a difference in frequencies between mouse and human cells?

Answer: Compare mean and covariance between the two.



## 8. Discussion

can we give a value for accuracy of the proposed algorithms?

Discuss limitations

### 8.1. Outlook

better frequency analysis (look into what causes these oscillations)

apply discussed algorithm to enough data to give good approximations of average and standard deviation to hold for arbitrary data sets



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## A. Python Implementation

We give a minimal version of the algorithm and code described in this work in Python.

```
1 import time
2 import math
3 import scipy
4 import numpy as np
5 import pandas as pd
6 from sklearn.mixture import GaussianMixture
7 from sklearn.cluster import KMeans
8 from sklearn.preprocessing import StandardScaler
9
10
11 def progress_bar(iterable, prefix=""):
12     start = time.time()
13     for i, item in enumerate(iterable):
14         yield item
15         print(f'\r{prefix}{i}/{len(iterable)}', end='', flush=True)
16     min, sec = divmod(time.time()-start, 60)
17     print(f"\r{prefix} took {int(min): 02}min {sec: 03.1f}s")
18
19
20 def approximate(dataframe):
21     def calc_t(w, k, alpha=0.99):
22         tmp = 1 / alpha - 1
23         if tmp < 0.0001:
24             return None
25         try:
26             return w - math.log(tmp) / k
27         except ValueError:
28             return None
29
30     def approx_func_(x, w1, t, w2, a, d, u, k1, k2):
31         if t is None: # transition point lies outside datapoints
32             return u
33         elif x <= t: # logistic function before transition point
34             tmp = -k1 * (x - w1)
35             if tmp <= 32:
36                 res = (a - u) / (1 + math.exp(tmp))
37             else:
38                 res = 0
39             return res + u
40         else: # logistic function after transition point
41             tmp = -k2 * (x - w2)
42             if tmp <= 32:
43                 res = (a - d) / (1 + math.exp(tmp))
44             else:
45                 res = 0
```

```
46         return res + d
47
48     def approx_func(x_arr, w1_start, w2_w1, a_d, d_u, u, k1, k2):
49         w1 = w1_start + start
50         w2 = w2_w1 + w1
51         d = d_u + u
52         a = a_d + d
53         transition_point = calc_t(w1, k1)
54         return (np.vectorize(approx_func_)
55                 (x_arr, w1, transition_point, w2, a, d, u, k1, k2))
56
57     min_val = np.min(dataframe['ratio'])
58     median_val = np.median(dataframe['ratio'])
59     max_val = np.max(dataframe['ratio'])
60     start, end = min(dataframe['frame']), max(dataframe['frame'])
61
62     lower_bounds = (0, 0, 0, 0, min_val, 0.05, -1)
63     upper_bounds = (end - start, end - start, max_val, max_val,
64                     max_val, 3, -0.01)
65     p0 = (0, (end - start) / 2, max_val - median_val, median_val - min_val,
66           min_val, 0.1, -0.03)
67
68     popt, *_ = scipy.optimize.curve_fit(approx_func, dataframe['frame'],
69                                         dataframe['ratio'], p0=p0,
70                                         method='trf',
71                                         bounds=(lower_bounds, upper_bounds))
72
73     w1_start, w2_w1, a_d, d_u, u, k1, k2 = popt
74     w1 = w1_start + start
75     w2 = w2_w1 + w1
76     d = d_u + u
77     a = a_d + d
78     t = calc_t(w1, k1)
79     return {"a": a, "u": u, "d": d, "k1": k1, "k2": k2, "w1": w1, "w2": w2}
80
81
82 def approximation_loop(file_name):
83     data = pd.DataFrame(pd.read_hdf(f"../data/{file_name}"))
84
85     # filter data
86     data = data[np.isfinite(data["ratio"])]
87     data = data[np.less(data["ratio"], np.full((len(data["ratio"])), 5))]
88     data = data[np.greater(data["ratio"], np.full((len(data["ratio"])), 0))]
89
90     all_parameters = list()
91     parameters_saved = ["idx", "a", "u", "d", "k1", "k2", "w1", "w2"]
92
93     for particle_idx in progress_bar(set(data['particle']),
94                                     f"approx {file_name}: "):
95         single_particle_data = (
96             data.loc[data['particle'] == particle_idx][['frame', 'ratio']]
97
98         # skip if too few datapoints
99         if len(single_particle_data['frame']) < 300:
100             continue
```

---

```

101
102     try: # throws error if no best fit was found
103         parameters = approximate(single_particle_data)
104
105         parameters["idx"] = str(particle_idx) + file_name
106         all_parameters.append([parameters[e] for e in parameters_saved])
107
108     except Exception as e:
109         print(f"\nerror in particle {particle_idx}: {e}")
110
111     return pd.DataFrame(all_parameters, columns=parameters_saved)
112
113
114 def normalize(neg_df, pos_df, exp_df, normalized_columns):
115     all_data = pd.concat([neg_df, pos_df, exp_df])
116
117     scaler = StandardScaler()
118     all_data[normalized_columns] = (scaler.fit_transform(
119         all_data[normalized_columns]))
120
121     neg_df = all_data[all_data["idx"].isin(neg_df["idx"])]
122     pos_df = all_data[all_data["idx"].isin(pos_df["idx"])]
123     exp_df = all_data[all_data["idx"].isin(exp_df["idx"])]
124
125     return neg_df, pos_df, exp_df
126
127
128 def remove_outliers(data, width, par_used):
129     for par in set(par_used):
130         mean, std = data[par].mean(), data[par].std()
131         data = data.drop(data[(data[par] <= mean - std * width) &
132                               (data[par] >= mean + std * width)].index)
133
134     return data
135
136 def separate(neg_df, pos_df, prediction_parameters, clustering_method):
137     neg_df["activation"] = "negative"
138     pos_df["activation"] = "positive"
139     data = pd.concat([neg_df, pos_df])
140
141     # clustering
142     if clustering_method == "gaussian_mixture":
143         clustering = GaussianMixture(n_components=2, covariance_type="diag",
144                                     n_init=10)
145     elif clustering_method == "kmeans":
146         clustering = KMeans(n_clusters=2, n_init=10)
147     else:
148         raise RuntimeError(f"Value of CLUSTERING_METHOD set to "
149                             f"{clustering_method}, which is not one of "
150                             f"[gaussian_mixture, kmeans].")
151     data["predicted"] = clustering.fit_predict(data[prediction_parameters])
152
153     # find association between predicted clusters and files
154     neg_0 = len(data[(data['predicted'] == 0) &
155                     (data['activation'] == "negative")])

```

```
156     neg_1 = len(data[(data['predicted'] == 1) &
157                     (data['activation'] == "negative")])
158     pos_0 = len(data[(data['predicted'] == 0) &
159                     (data['activation'] == "positive")])
160     pos_1 = len(data[(data['predicted'] == 1) &
161                     (data['activation'] == "positive")])
162
163     permutation = (0, 1) if neg_0 + pos_1 > neg_1 + pos_0 else (1, 0)
164
165     return permutation, clustering
166
167
168 if __name__ == "__main__":
169     FILE_NAME_NEG_CONTROL = "mouse_negative/mouse_negative.h5"
170     FILE_NAME_POS_CONTROL = "mouse_positive/mouse_positive.h5"
171     FILE_NAME_EXPERIMENT = "mouse_experiment/mouse_experiment.h5"
172
173     USED_COLUMNS = ["a", "u", "d", "k1", "k2", "w1", "w2"]
174     CLUSTERING_METHOD = "gaussian_mixture" # gaussian_mixture or kmeans
175
176     print(f"Using {CLUSTERING_METHOD} on files {FILE_NAME_NEG_CONTROL}, "
177           f"{FILE_NAME_POS_CONTROL} and {FILE_NAME_EXPERIMENT} with "
178           f"parameters {USED_COLUMNS}.\n")
179
180     neg_df = approximation_loop(FILE_NAME_NEG_CONTROL)
181     pos_df = approximation_loop(FILE_NAME_POS_CONTROL)
182     exp_df = approximation_loop(FILE_NAME_EXPERIMENT)
183
184     n = min(len(neg_df), len(pos_df))
185     neg_df, pos_df = neg_df.sample(n), pos_df.sample(n)
186
187     neg_df, pos_df, exp_df = normalize(neg_df, pos_df, exp_df, USED_COLUMNS)
188
189     neg_df = remove_outliers(neg_df, 3, USED_COLUMNS)
190     pos_df = remove_outliers(pos_df, 3, USED_COLUMNS)
191     exp_df = remove_outliers(exp_df, 3, USED_COLUMNS)
192
193     per, clustering = separate(neg_df, pos_df, USED_COLUMNS,
194                               CLUSTERING_METHOD)
195
196     neg_df["predicted"] = clustering.predict(neg_df[USED_COLUMNS])
197     pos_df["predicted"] = clustering.predict(pos_df[USED_COLUMNS])
198     exp_df["predicted"] = clustering.predict(exp_df[USED_COLUMNS])
199
200     neg_act = len(neg_df[neg_df['predicted'] == per[1]])
201     pos_act = len(pos_df[pos_df['predicted'] == per[1]])
202     exp_act = len(exp_df[exp_df['predicted'] == per[1]])
203     neg_len, pos_len, exp_len = len(neg_df), len(pos_df), len(exp_df)
204
205     print("\nfile: activated      out of      percentage")
206     print(f"neg:  {neg_act:<13} {neg_len:<10} {neg_act/neg_len * 100:.3f}")
207     print(f"pos:  {pos_act:<13} {pos_len:<10} {pos_act/pos_len * 100:.3f}")
208     print(f"exp:  {exp_act:<13} {exp_len:<10} {exp_act/exp_len * 100:.3f}")
```