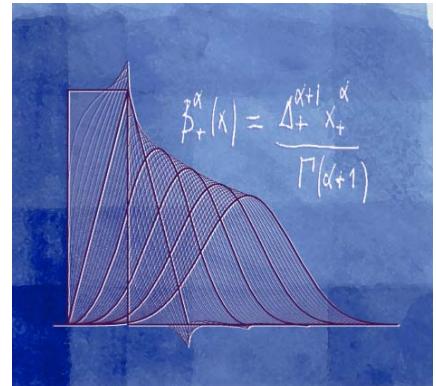


# Hybrid sparse stochastic processes and the resolution of linear inverse problems

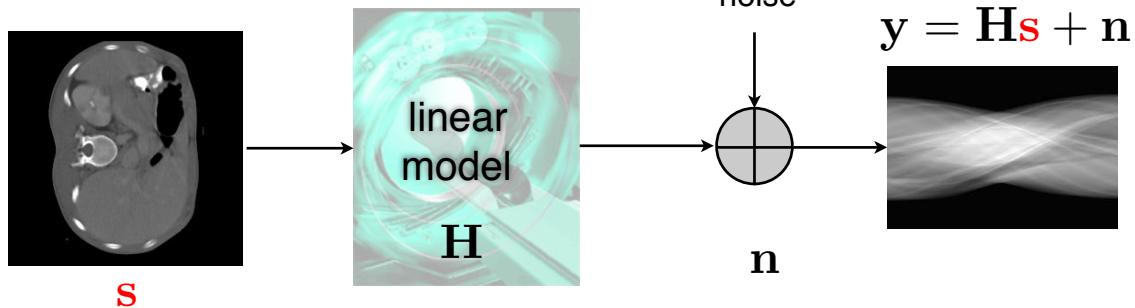
Michael Unser  
Biomedical Imaging Group  
EPFL, Lausanne, Switzerland



*Statistical Models for Shape and Imaging*, March 11-15, 2019, Institut Poincaré, Paris

## Variational-MAP formulation of inverse problem

- Linear forward model



- Reconstruction as an optimization problem

$$\mathbf{s}_{\text{rec}} = \arg \min \underbrace{\|\mathbf{y} - \mathbf{Hs}\|_2^2}_{\text{data consistency}} + \underbrace{\lambda \|\mathbf{Ls}\|_p^p}_{\text{regularization}}, \quad p = 1, 2$$

–  $-\log \text{Prob}(\mathbf{s})$  : prior likelihood

# An introduction to sparse stochastic processes

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## Random spline: archetype of sparse signal

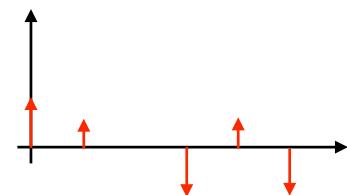
Random weights  $\{a_n\}$  i.i.d. and random knots  $\{t_n\}$  (Poisson with rate  $\lambda$ )

### ■ Stochastic differential equation

$$Ds(t) = w(t)$$

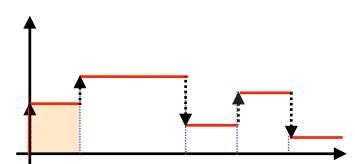
with boundary condition  $s(0) = 0$

**Innovation:**  $w(t) = \sum_n a_n \delta(t - t_n)$



### ■ Formal solution = Compound Poisson process

$$\begin{aligned} s(t) &= D^{-1}w(t) = \sum_n a_n D^{-1}\{\delta(\cdot - t_n)\}(t) \\ &= b_1 + \sum_n a_n \mathbb{1}_+(t - t_n) \end{aligned}$$

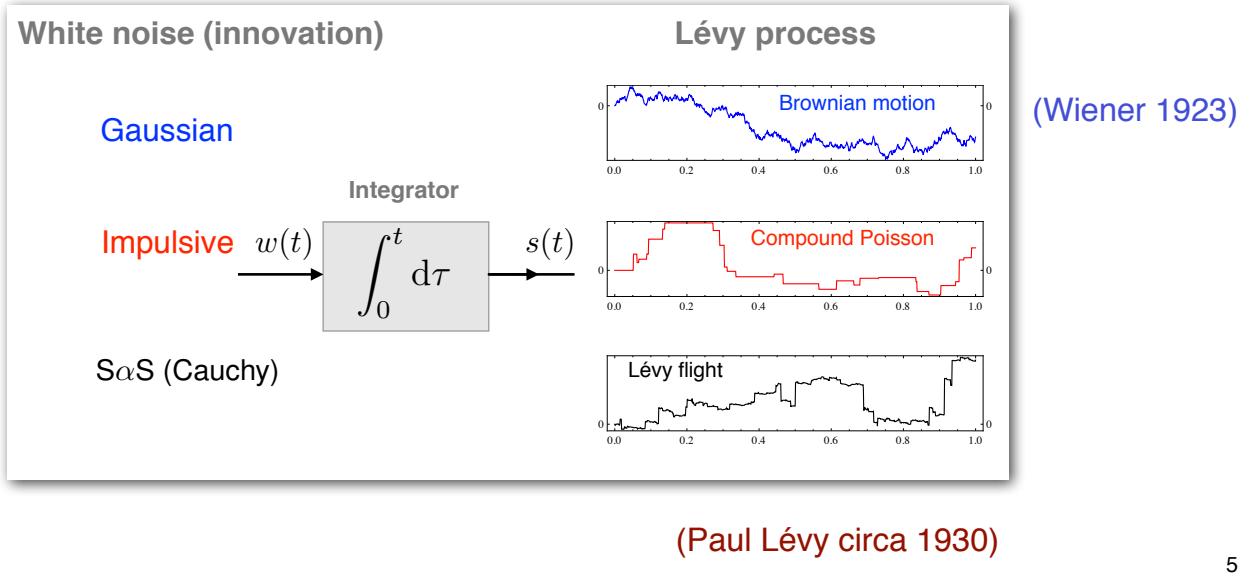


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# Lévy processes: all admissible brands of innovations

Generalized innovations : white Lévy noise with  $\mathbb{E}\{w(t)w(t')\} = \sigma_w^2 \delta(t - t')$

$$Ds = w \quad (\text{perfect decoupling!}) \quad \in \mathcal{S}'(\mathbb{R}^d)$$

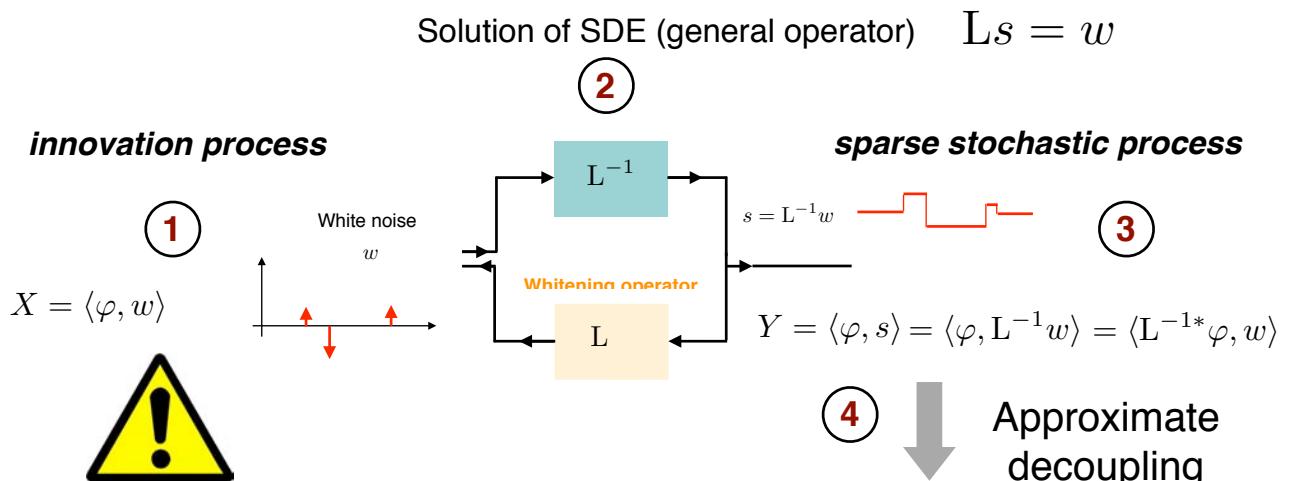


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## Generalized innovation model

Theoretical framework: Gelfand's theory of **generalized stochastic processes**

Generic test function  $\varphi \in \mathcal{S}(\mathbb{R}^d)$  plays the role of index variable



Proper definition of  
**continuous-domain** white noise

(Unser et al, IEEE-IT 2014)

**Regularization operator vs. wavelet analysis**

**Main feature: inherent sparsity**  
(few significant coefficients)

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# Description of sparse stochastic process

## ■ Specification of spatial dependencies

$$\text{Whitening operator } L \Rightarrow s = L^{-1}w \in \mathcal{S}'(\mathbb{R}^d)$$

## ■ Specification of innovation (sparsity behavior)

Canonical observation through a rectangular window

$$X_{\text{id}} = \langle w, \text{rect} \rangle = \langle \text{white noise}, \text{rectangular window} \rangle$$

$w = \text{white noise} \Rightarrow X_{\text{id}} = \langle w, \text{rect} \rangle$  is **infinitely divisible**  
with **canonical Lévy exponent**  $f(\omega) = \log \mathbb{E}\{e^{j\omega X_{\text{id}}}\}$ .

**Definition:** A random variable  $X$  with generic pdf  $p_{\text{id}}(x)$  is **infinitely divisible (id)** iff., for any  $N \in \mathbb{Z}^+$ , there exist i.i.d. random variables  $X_1, \dots, X_N$  such that  $X \stackrel{d}{=} X_1 + \dots + X_N$ .

$$\begin{aligned} X = \langle w, \text{rect} \rangle &= \langle \text{white noise}, \text{rectangular window} \rangle \\ &= \langle \text{white noise}, \frac{1}{n} \text{ window} \rangle + \dots + \langle \text{white noise}, \frac{1}{n} \text{ window} \rangle \end{aligned}$$

i.i.d.

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## ⇒ Probability laws of sparse processes are id

### ■ Analysis: go back to **innovation process**: $w = Ls$

■ Generic random observation:  $X = \langle \varphi, w \rangle$  with  $\varphi \in \mathcal{S}(\mathbb{R}^d)$  or  $\varphi \in L_p(\mathbb{R}^d)$  (by extension)

■ Linear functional:  $Y = \langle \psi, s \rangle = \langle \psi, L^{-1}w \rangle = \langle L^{-1}\psi, w \rangle$

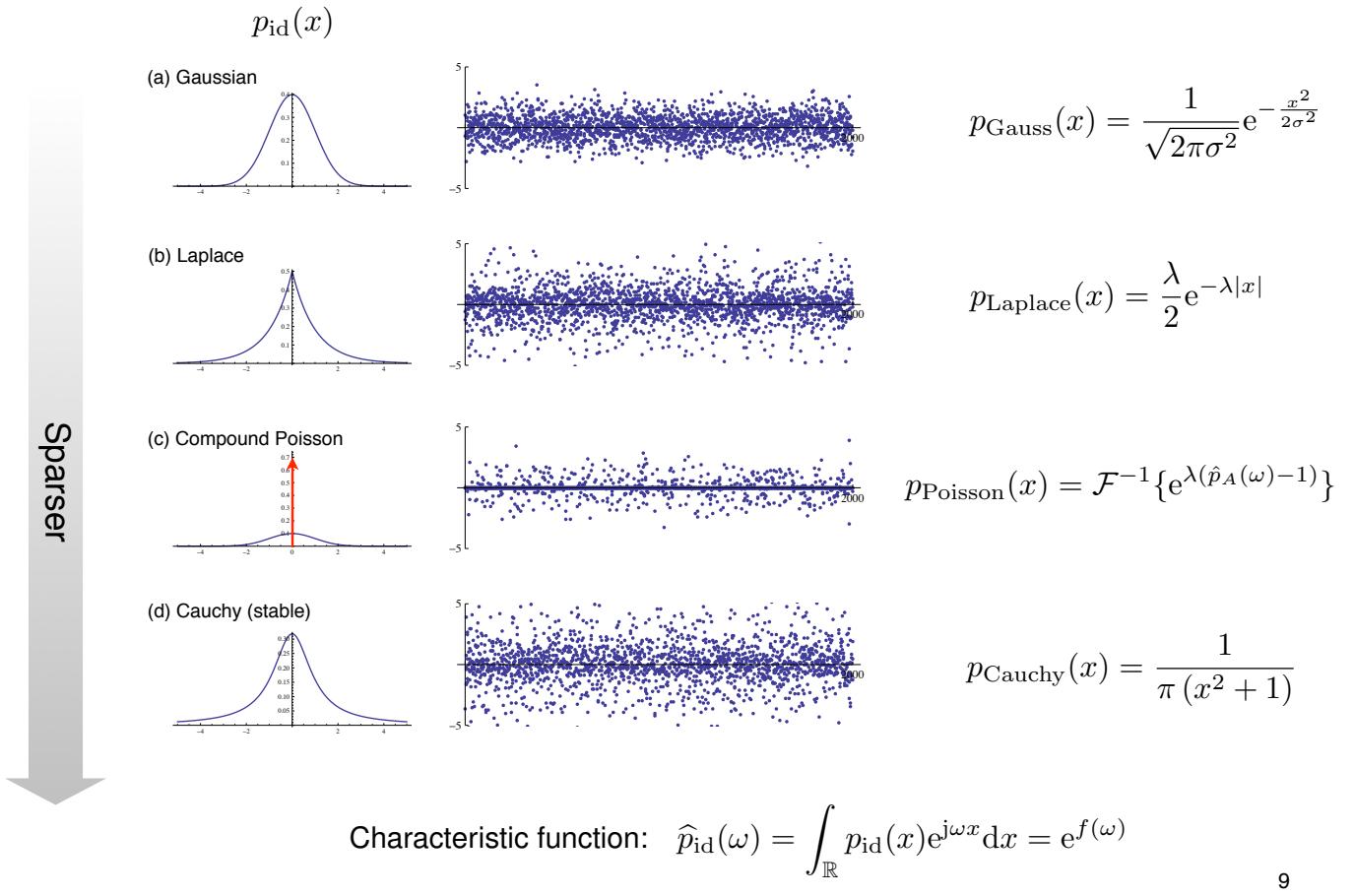
If  $\phi = L^{-1}\psi \in L_p(\mathbb{R}^d)$  then  $Y = \langle \psi, s \rangle = \langle \phi, w \rangle$  is **infinitely divisible**  
with (modified) **Lévy exponent**  $f_\phi(\omega) = \int_{\mathbb{R}^d} f(\omega\phi(x))dx$

$$\Rightarrow p_Y(y) = \mathcal{F}^{-1}\{e^{f_\phi(\omega)}\}(y) = \int_{\mathbb{R}} e^{f_\phi(\omega) - j\omega y} \frac{d\omega}{2\pi}$$



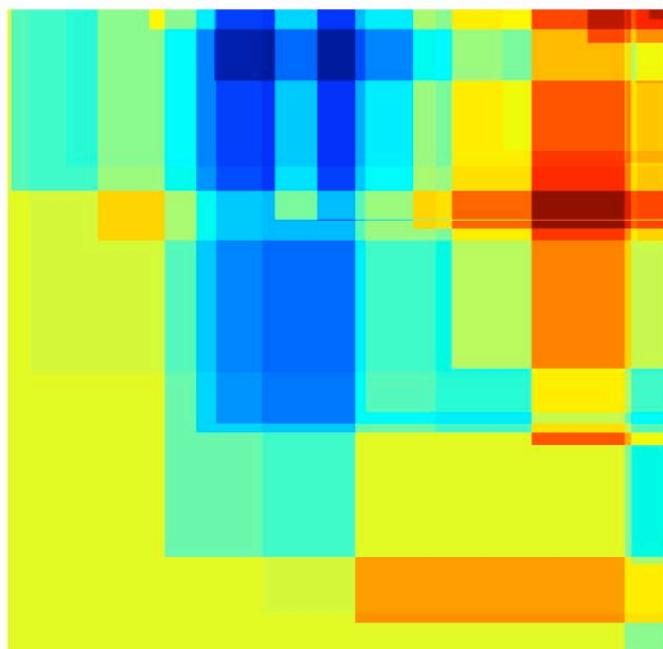
= explicit form of pdf

# Examples of infinitely divisible laws



## Aesthetic sparse signal: the Mondrian process

$$L = D_x D_y \quad \longleftrightarrow \quad (j\omega_x)(j\omega_y)$$



## High-level properties of SSP

- **Infinite divisible probability laws:** broadest class of distributions preserved through linear transformation.
- **Explicit calculations:** Analytical determination of transform-domain statistics (including, joint pdfs).
- **Unifying framework:** includes all traditional families of stochastic processes (ARMA, fBm), as well as their non-Gaussian generalizations.
- **Sparsifying transforms / ICA:** SSP are (approximately) decoupled in a matched operator-like wavelet basis. (Pad-U., IEEE-SP 2015)
- **$N$ -term approximation properties:** SSP are truly “sparse” as described by their inclusion in (weighted) Besov spaces. (Fageot et al., ACHA 2015)



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## OUTLINE

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- Non-Gaussian statistical modeling ✓
  - Sparse stochastic processes
- Hybrid sparse stochastic processes
- Iterative image reconstruction (MAP formulation)

# Hybrid stochastic processes

■ Hybrid sparse processes:  $s_{\text{hyb}} = s_1 + \dots + s_I$

■ Description of independent components

■ Innovation model:  $\mathbf{L}_i s_i = \mathbf{w}_i \Rightarrow s_i = \mathbf{L}_i^{-1} \mathbf{w}_i$

■ Whitening operator:  $\mathbf{L}_i : \mathcal{S}'(\mathbb{R}^d) \rightarrow \mathcal{S}'(\mathbb{R}^d)$

■ Lévy exponent of white noise:  $f_i : \mathbb{R} \rightarrow \mathbb{C}$

■ Characteristic functionals  $\widehat{\mathcal{P}}_{\mathbf{w}_i}, \widehat{\mathcal{P}}_{s_i} : \mathcal{S}(\mathbb{R}^d) \rightarrow \mathbb{C}$

$$\widehat{\mathcal{P}}_{\mathbf{w}_i}(\varphi) \triangleq \mathbb{E}\{e^{j\langle \mathbf{w}_i, \varphi \rangle}\} = \exp\left(\int_{\mathbb{R}^d} f_i(\varphi(\mathbf{x})) d\mathbf{x}\right)$$

$$\widehat{\mathcal{P}}_{s_i}(\varphi) = \mathbb{E}\{e^{j\langle s_i, \varphi \rangle}\} = \mathbb{E}\{e^{j\langle \mathbf{L}_i^{-1} \mathbf{w}_i, \varphi \rangle}\} = \mathbb{E}\{e^{j\langle \mathbf{w}_i, \mathbf{L}_i^{-1*} \varphi \rangle}\} = \widehat{\mathcal{P}}_{\mathbf{w}_i}(\mathbf{L}_i^{-1*} \varphi)$$

$$\widehat{\mathcal{P}}_{s_{\text{hyb}}}(\varphi) = \prod_{i=1}^I \widehat{\mathcal{P}}_{s_i}(\varphi) = \exp\left(\int_{\mathbb{R}^d} \sum_{i=1}^I f_i(\mathbf{L}_i^{-1*} \varphi(\mathbf{x})) d\mathbf{x}\right)$$

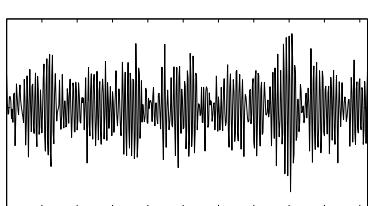
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## Hybrid processes: Audio signal modeling

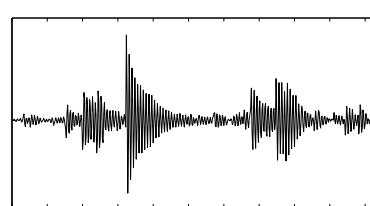
■ Sparse, bandpass processes

poles = [-.05 + jπ/2, -.05 - jπ/2], zeros = []

$$L = \frac{d^n}{dt^n} + a_{n-1} \frac{d^{n-1}}{dt^{n-1}} + \dots + a_1 \frac{d}{dt} + a_0 I$$



(a) Gaussian



(b) Alpha stable  $\alpha=1.2$

■ Hybrid sparse processes:  $s_{\text{hyb}} = s_1 + \dots + s_I$

$$\widehat{\mathcal{P}}_{s_{\text{hyb}}}(\varphi) = \prod_{i=1}^I \widehat{\mathcal{P}}_{s_i}(\varphi) = \exp\left(\int_{\mathbb{R}} \sum_{i=1}^I f_i(\mathbf{L}_i^{-1*} \varphi(t)) dt\right)$$



Gaussian (Am)



generalized Lévy (Am, SαS)

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# Discretization of linear inverse problem

$$s(\mathbf{r}) = \sum_{\mathbf{k} \in \Omega} s[\mathbf{k}] \beta_{\mathbf{k}}(\mathbf{r}) \quad s(\mathbf{r}) = \sum_{i=1}^I s_i(\mathbf{r}): \text{hybrid sparse process}$$

Partial signals and innovation vectors:  $\mathbf{s}_i = (s_i[\mathbf{k}])_{\mathbf{k} \in \Omega}$  and  $\mathbf{u}_i = (u[\mathbf{k}])_{\mathbf{k} \in \Omega}$  of dimension  $K$

- Discrete innovation model

$$\mathbf{u}_i = \mathbf{L}_i \mathbf{s}_i \quad \mathbf{L}_i: (K \times K) \text{ matrix representation of } \mathbf{L}_{i,d}$$

- Measurement model (image formation)

$$y_m = \int_{\mathbb{R}^d} s(\mathbf{r}) \eta_m(\mathbf{r}) d\mathbf{r} + n[m] = \langle s, \eta_m \rangle + n[m], \quad (m = 1, \dots, M)$$

$\eta_m$ : sampling/imaging function ( $m$ th detector)

$n[\cdot]$ : additive i.i.d. noise with pdf  $p_N$

$$\mathbf{y} = \mathbf{y}_0 + \mathbf{n} = \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I) + \mathbf{n}$$

$$(M \times K) \text{ system matrix : } [\mathbf{H}]_{m,\mathbf{k}} = \langle \eta_m, \beta_{\mathbf{k}} \rangle = \int_{\mathbb{R}^d} \eta_m(\mathbf{r}) \beta_{\mathbf{k}}(\mathbf{r}) d\mathbf{r}$$

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# Posterior probability distribution

$$\begin{aligned} p_{S|Y}(\mathbf{s}_1, \dots, \mathbf{s}_I | \mathbf{y}) &= \frac{p_{Y|S}(\mathbf{y} | \mathbf{s}_1, \dots, \mathbf{s}_I) p_S(\mathbf{s}_1, \dots, \mathbf{s}_I)}{p_Y(\mathbf{y})} && \text{(Bayes' rule)} \\ &= \frac{p_N(\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)) p_S(\mathbf{s}_1, \dots, \mathbf{s}_I)}{p_Y(\mathbf{y})} \\ &= \frac{1}{Z} p_N(\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)) p_S(\mathbf{s}_1, \dots, \mathbf{s}_I) \end{aligned}$$

$$\text{Independence of partial signals: } p_S(\mathbf{s}_1, \dots, \mathbf{s}_I) = \prod_{i=1}^I p_S(\mathbf{s}_i)$$

$$\text{Innovation model: } \mathbf{u}_i = \mathbf{L}_i \mathbf{s}_i \quad \Rightarrow \quad p_S(\mathbf{s}_i) \propto p_{U_i}(\mathbf{L}_i \mathbf{s}_i)$$

$$\begin{aligned} p_{S|Y}(\mathbf{s}_1, \dots, \mathbf{s}_I | \mathbf{y}) &\propto p_N(\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)) \prod_{i=1}^I p_{U_i}(\mathbf{u}_i) && \text{(decoupling simplification)} \\ &\approx p_N(\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)) \prod_{\mathbf{k} \in \Omega} \prod_{i=1}^I p_{U_i}([\mathbf{L}_i \mathbf{s}_i]_{\mathbf{k}}) \end{aligned}$$

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# Statement of MAP reconstruction problem

## ■ Hypotheses

$$\mathbf{y} = \mathbf{H}\mathbf{s} + \mathbf{n} \text{ where } \mathbf{n} \text{ AWGN with variance } \sigma^2$$

$\mathbf{s} = \mathbf{s}_1 + \dots + \mathbf{s}_I$  (sum of independent sparse processes)

$\mathbf{L}_i \mathbf{s}_i = \mathbf{u}_i$ : i.i.d. with pdf  $p_{U_i}$  and id potential function  $\Phi_{U_i}(x) \triangleq -\log p_{U_i}(x)$

## ■ Additive white Gaussian noise scenario (AWGN)

$$p_{S|Y}(\mathbf{s}_1, \dots, \mathbf{s}_I | \mathbf{y}) \propto \exp\left(-\frac{\|\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)\|^2}{2\sigma^2}\right) \prod_{k \in \Omega} \prod_{i=1}^I p_{U_i}([\mathbf{L}_i \mathbf{s}_i]_k)$$

## ■ Maximum a posteriori (MAP) estimator

$$\begin{aligned} \arg \min_{\mathbf{s}_1, \dots, \mathbf{s}_I \in \mathbb{R}^K} & \left( \frac{1}{2\sigma^2} \|\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)\|_2^2 \right. \\ & \left. + \sum_{k \in \Omega} \Phi_{U_1}([\mathbf{L}_1 \mathbf{s}_1]_k) + \dots + \sum_{k \in \Omega} \Phi_{U_I}([\mathbf{L}_I \mathbf{s}_I]_k) \right) \end{aligned}$$

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# Hybrid model: reformulation

$$\begin{aligned} \arg \min_{\mathbf{s}_1, \dots, \mathbf{s}_I \in \mathbb{R}^K} & \left( \frac{1}{2\sigma^2} \|\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \dots + \mathbf{s}_I)\|_2^2 \right. \\ & \left. + \sum_{k \in \Omega} \Phi_{U_1}([\mathbf{L}_1 \mathbf{s}_1]_k) + \dots + \sum_{k \in \Omega} \Phi_{U_I}([\mathbf{L}_I \mathbf{s}_I]_k) \right) \end{aligned}$$

## ■ Augmented formulation of the problem

- **Unmixed** signal:  $\mathbf{s} = (\mathbf{s}_1, \dots, \mathbf{s}_I) \in \mathbb{R}^{K \times I}$
- Augmented **innovation**:  $\mathbf{u} = (\mathbf{u}_1, \dots, \mathbf{u}_I) \in \mathbb{R}^{K \times I}$
- Augmented system matrix:  $\mathbf{H}_{\text{aug}} = [\mathbf{H} \cdots \mathbf{H}] \in \mathbb{R}^{M \times KI}$
- Augmented whitening operator:  $\mathbf{L}_{\text{aug}} = \text{diag}(\mathbf{L}_1, \dots, \mathbf{L}_I) \in \mathbb{R}^{KI \times KI}$

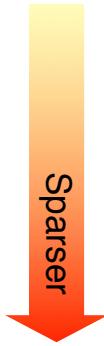
$$\arg \min_{\mathbf{s} \in \mathbb{R}^{IK}} \left( \frac{1}{2\sigma^2} \|\mathbf{y} - \mathbf{H}_{\text{aug}} \mathbf{s}\|_2^2 + \sum_n \Phi_{U_n}([\mathbf{u}]_n) \right) \quad \text{s.t.} \quad \mathbf{u} = \mathbf{L}_{\text{aug}} \mathbf{s}$$

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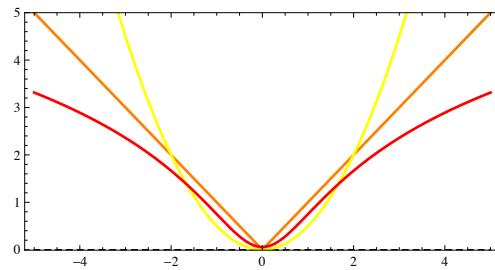
## General form of MAP estimator (hybrid)

$$\mathbf{s}_{\text{MAP}} = \operatorname{argmin} \left( \frac{1}{2} \|\mathbf{y} - \mathbf{H}_{\text{aug}} \mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_{U_n}([\mathbf{L}_{\text{aug}} \mathbf{s}]_n) \right)$$

- Gaussian:  $p_U(x) = \frac{1}{\sqrt{2\pi}\sigma_0} e^{-x^2/(2\sigma_0^2)}$   $\Rightarrow \Phi_U(x) = \frac{1}{2\sigma_0^2}x^2 + C_1$
- Laplace:  $p_U(x) = \frac{\lambda}{2} e^{-\lambda|x|}$   $\Rightarrow \Phi_U(x) = \lambda|x| + C_2$
- Student:  $p_U(x) = \frac{1}{B(r, \frac{1}{2})} \left( \frac{1}{x^2 + 1} \right)^{r+\frac{1}{2}}$   $\Rightarrow \Phi_U(x) = \left( r + \frac{1}{2} \right) \log(1 + x^2) + C_3$



Potential:  $\Phi_U(x) = -\log p_U(x)$

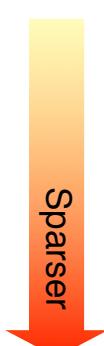


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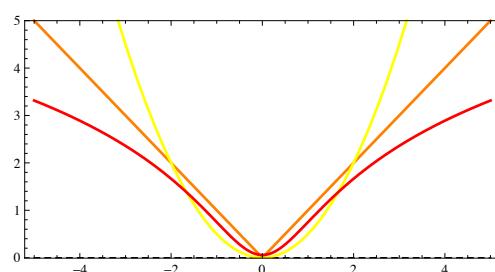
## General form of MAP estimator (standard)

$$\mathbf{s}_{\text{MAP}} = \operatorname{argmin} \left( \frac{1}{2} \|\mathbf{y} - \mathbf{H} \mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_U([\mathbf{L} \mathbf{s}]_n) \right)$$

- Gaussian:  $p_U(x) = \frac{1}{\sqrt{2\pi}\sigma_0} e^{-x^2/(2\sigma_0^2)}$   $\Rightarrow \Phi_U(x) = \frac{1}{2\sigma_0^2}x^2 + C_1$
- Laplace:  $p_U(x) = \frac{\lambda}{2} e^{-\lambda|x|}$   $\Rightarrow \Phi_U(x) = \lambda|x| + C_2$
- Student:  $p_U(x) = \frac{1}{B(r, \frac{1}{2})} \left( \frac{1}{x^2 + 1} \right)^{r+\frac{1}{2}}$   $\Rightarrow \Phi_U(x) = \left( r + \frac{1}{2} \right) \log(1 + x^2) + C_3$



Potential:  $\Phi_U(x) = -\log p_U(x)$

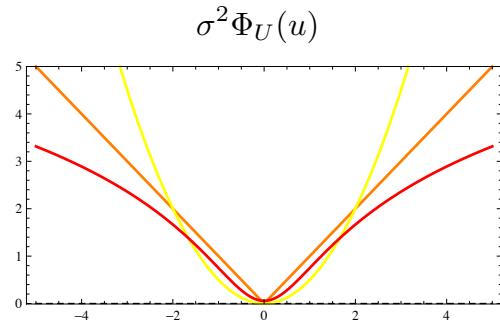
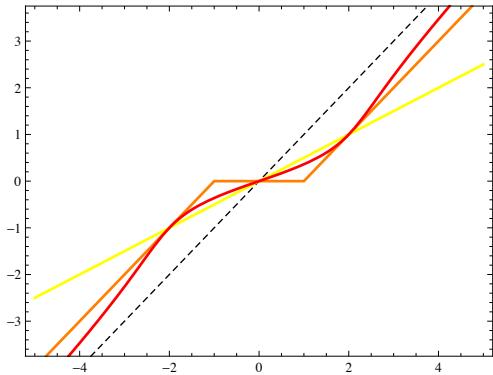


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## Proximal operator: pointwise denoiser

$$\text{prox}_{\Phi_U}(y; \sigma^2) = \arg \min_{u \in \mathbb{R}} \frac{1}{2} |y - u|^2 + \sigma^2 \Phi_U(u)$$

$$\tilde{u} = \text{prox}_{\Phi_U}(y; 1)$$



- linear attenuation                               $\ell_2$  minimization
- soft-threshold                                   $\ell_1$  minimization
- shrinkage function                               $\approx \ell_p$  relaxation for  $p \rightarrow 0$

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## Maximum a posteriori (MAP) estimation

- Constrained optimization formulation

Auxiliary **innovation** variable:  $\mathbf{u} = \mathbf{L}\mathbf{s}$

$$\mathbf{s}_{\text{MAP}} = \arg \min_{\mathbf{s} \in \mathbb{R}^K} \left( \frac{1}{2} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_U([\mathbf{u}]_n) \right) \text{ subject to } \mathbf{u} = \mathbf{L}\mathbf{s}$$

- Augmented Lagrangian method

Quadratic penalty term:  $\frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2$

Lagrange multiplier vector:  $\boldsymbol{\alpha}$

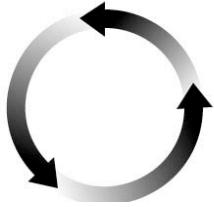
$$\mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}, \boldsymbol{\alpha}) = \frac{1}{2} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_U([\mathbf{u}]_n) + \boldsymbol{\alpha}^T (\mathbf{L}\mathbf{s} - \mathbf{u}) + \frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2$$

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# Alternating direction method of multipliers (ADMM)

$$\mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}, \boldsymbol{\alpha}) = \frac{1}{2} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_U([\mathbf{u}]_n) + \boldsymbol{\alpha}^T (\mathbf{L}\mathbf{s} - \mathbf{u}) + \frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2$$

Sequential minimization



$$\mathbf{s}^{k+1} \leftarrow \arg \min_{\mathbf{s} \in \mathbb{R}^N} \mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}^k, \boldsymbol{\alpha}^k)$$

$$\boldsymbol{\alpha}^{k+1} = \boldsymbol{\alpha}^k + \mu(\mathbf{L}\mathbf{s}^{k+1} - \mathbf{u}^k)$$

$$\mathbf{u}^{k+1} \leftarrow \arg \min_{\mathbf{u} \in \mathbb{R}^N} \mathcal{L}_{\mathcal{A}}(\mathbf{s}^{k+1}, \mathbf{u}, \boldsymbol{\alpha}^{k+1})$$

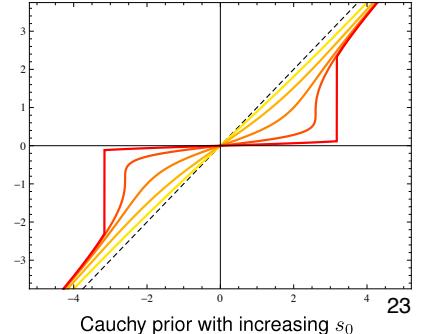
**Linear inverse problem:**  $\mathbf{s}^{k+1} = (\mathbf{H}^T \mathbf{H} + \mu \mathbf{L}^T \mathbf{L})^{-1} (\mathbf{H}^T \mathbf{y} + \mathbf{z}^{k+1})$

with  $\mathbf{z}^{k+1} = \mathbf{L}^T (\mu \mathbf{u}^k - \boldsymbol{\alpha}^k)$

**Nonlinear denoising:**  $\mathbf{u}^{k+1} = \text{prox}_{\Phi_U}(\mathbf{L}\mathbf{s}^{k+1} + \frac{1}{\mu} \boldsymbol{\alpha}^{k+1}; \frac{\sigma^2}{\mu})$

- Proximal operator taylored to stochastic model

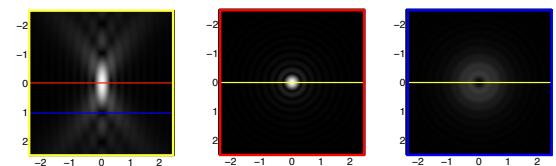
$$\text{prox}_{\Phi_U}(y; \lambda) = \arg \min_u \frac{1}{2} |y - u|^2 + \lambda \Phi_U(u)$$



# Deconvolution of fluorescence micrographs

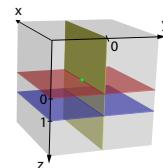
- Physical model of a diffraction-limited microscope

$$g(x, y, z) = (h_{3D} * s)(x, y, z)$$



3-D point spread function (PSF)

$$h_{3D}(x, y, z) = I_0 \left| p_\lambda \left( \frac{x}{M}, \frac{y}{M}, \frac{z}{M^2} \right) \right|^2$$

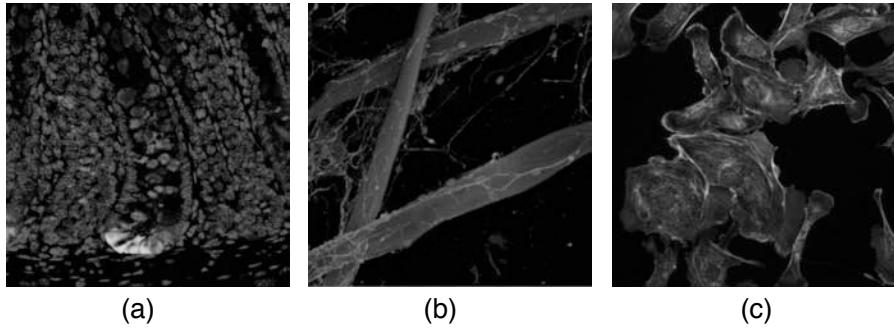


$$p_\lambda(x, y, z) = \int_{\mathbb{R}^2} P(\omega_1, \omega_2) \exp \left( j2\pi z \frac{\omega_1^2 + \omega_2^2}{2\lambda f_0^2} \right) \exp \left( -j2\pi \frac{x\omega_1 + y\omega_2}{\lambda f_0} \right) d\omega_1 d\omega_2$$

Optical parameters

- $\lambda$ : wavelength (emission)
- $M$ : magnification factor
- $f_0$ : focal length
- $P(\omega_1, \omega_2) = \mathbb{1}_{\|\omega\| < R_0}$ : pupil function
- $\text{NA} = n \sin \theta = R_0/f_0$ : numerical aperture

## Deconvolution experiments



**Figure 10.3** Images used in deconvolution experiments. (a) Stem cells surrounded by goblet cells. (b) Nerve cells growing around fibers. (c) Artery cells.

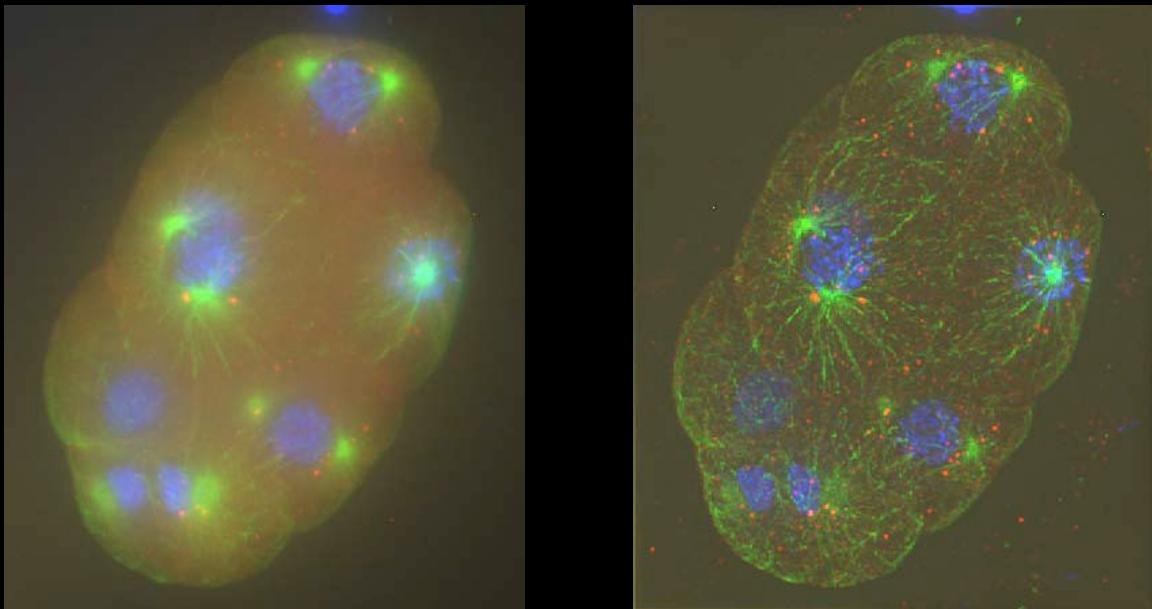
**Table 10.2** Deconvolution performance of MAP estimators based on different prior distributions.

	BSNR (dB)	Estimation performance (SNR in dB)		
		Gaussian	Laplace	Student's
Stem cells	20	<b>14.43</b>	13.76	11.86
	30	<b>15.92</b>	15.77	13.15
	40	<b>18.11</b>	<b>18.11</b>	13.83
Nerve cells	20	13.86	<b>15.31</b>	14.01
	30	15.89	<b>18.18</b>	15.81
	40	18.58	<b>20.57</b>	16.92
Artery cells	20	14.86	<b>15.23</b>	13.48
	30	16.59	<b>17.21</b>	14.92
	40	18.68	<b>19.61</b>	15.94

L: discrete gradient

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## 3D deconvolution with sparsity constraints



Maximum intensity projections of  $384 \times 448 \times 260$  image stacks;  
Leica DM 5500 widefield epifluorescence microscope with a  $63\times$  oil-immersion objective;  
C. Elegans embryo labeled with Hoechst, Alexa488, Alexa568;

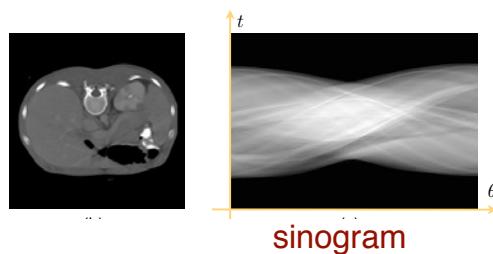
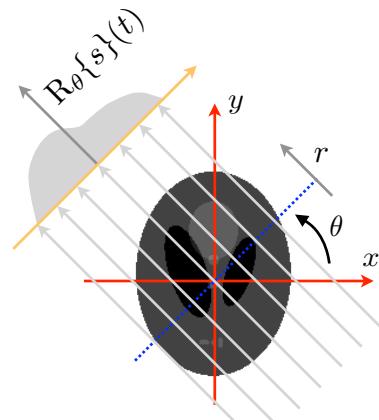
(Vonesch-U. *IEEE Trans. Im. Proc.* 2009)

# Computed tomography (straight rays)

Projection geometry:  $\mathbf{x} = t\theta + r\theta^\perp$  with  $\theta = (\cos \theta, \sin \theta)$

## ■ Radon transform (line integrals)

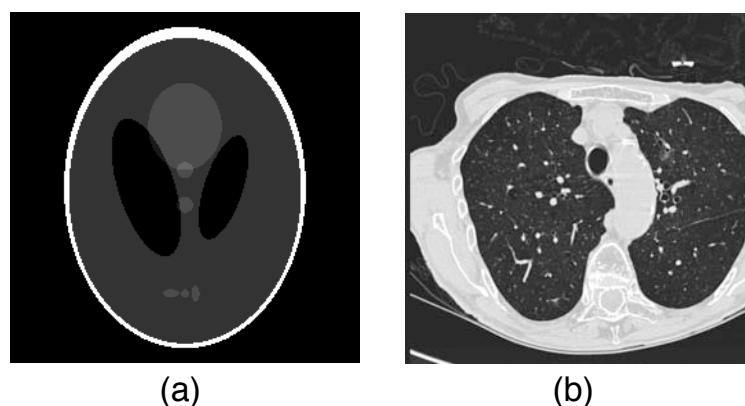
$$\begin{aligned} R_\theta\{s(\mathbf{x})\}(t) &= \int_{\mathbb{R}} s(t\theta + r\theta^\perp) dr \\ &= \int_{\mathbb{R}^2} s(\mathbf{x}) \delta(t - \langle \mathbf{x}, \theta \rangle) d\mathbf{x} \end{aligned}$$



Equivalent analysis functions:  $\eta_m(\mathbf{x}) = \delta(t_m - \langle \mathbf{x}, \theta_m \rangle)$

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# Computed tomography reconstruction results



**Figure 10.6** Images used in X-ray tomographic reconstruction experiments. (a) The Shepp-Logan (SL) phantom. (b) Cross section of a human lung.

**Table 10.4** Reconstruction results of X-ray computed tomography using different estimators.

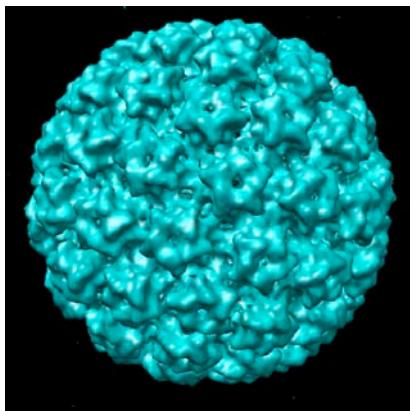
	Directions	Estimation performance (SNR in dB)			L: discrete gradient
		Gaussian	Laplace	Student's	
SL Phantom	120	16.8	17.53	<b>18.76</b>	
SL Phantom	180	18.13	18.75	<b>20.34</b>	
Lung	180	<b>22.49</b>	21.52	21.45	
Lung	360	<b>24.38</b>	22.47	22.37	

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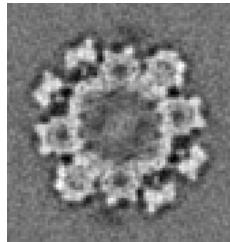
# Cryo-electron tomography (real data)



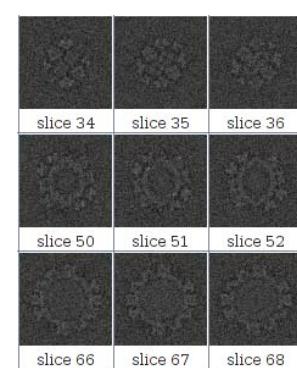
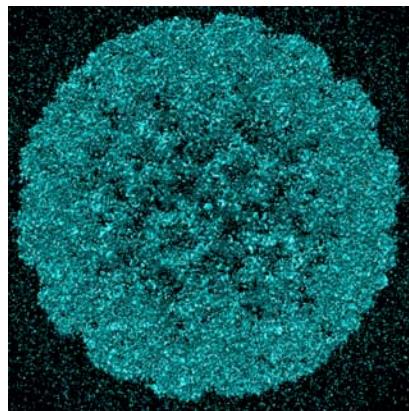
Standard Fourier-based reconstruction



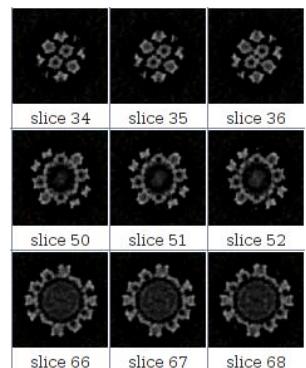
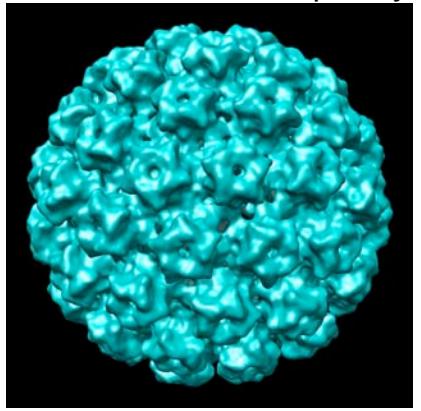
6.185 Å



High-resolution Fourier-based reconstruction



High-resolution reconstruction with sparsity



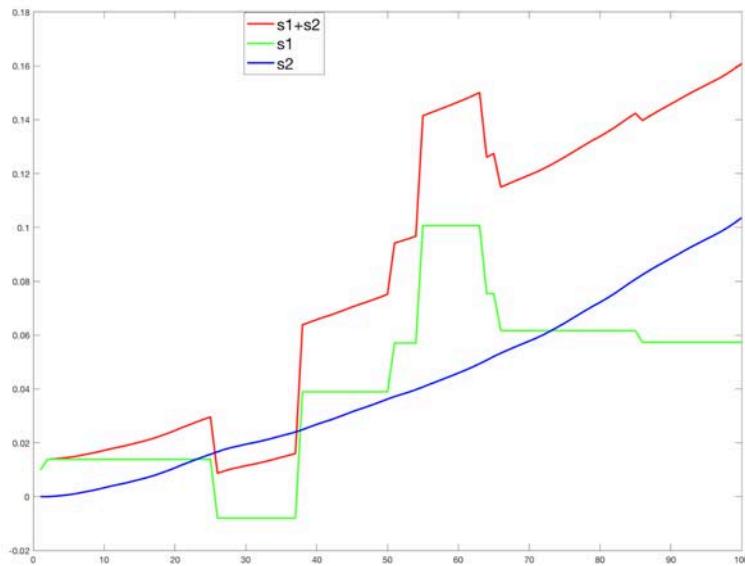
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## Hybrid Model

$$s = s_1 + s_2$$

$$L_1 = D, \quad w_1: \text{impulsive noise}$$

$$L_2 = D^2, \quad w_2: \text{Gaussian noise}$$



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# Fourier Sampling (1D MRI)

- Forward model: Quasi-random sampling in Fourier domain
- Denser sampling at low-frequencies
- Recovery methods:

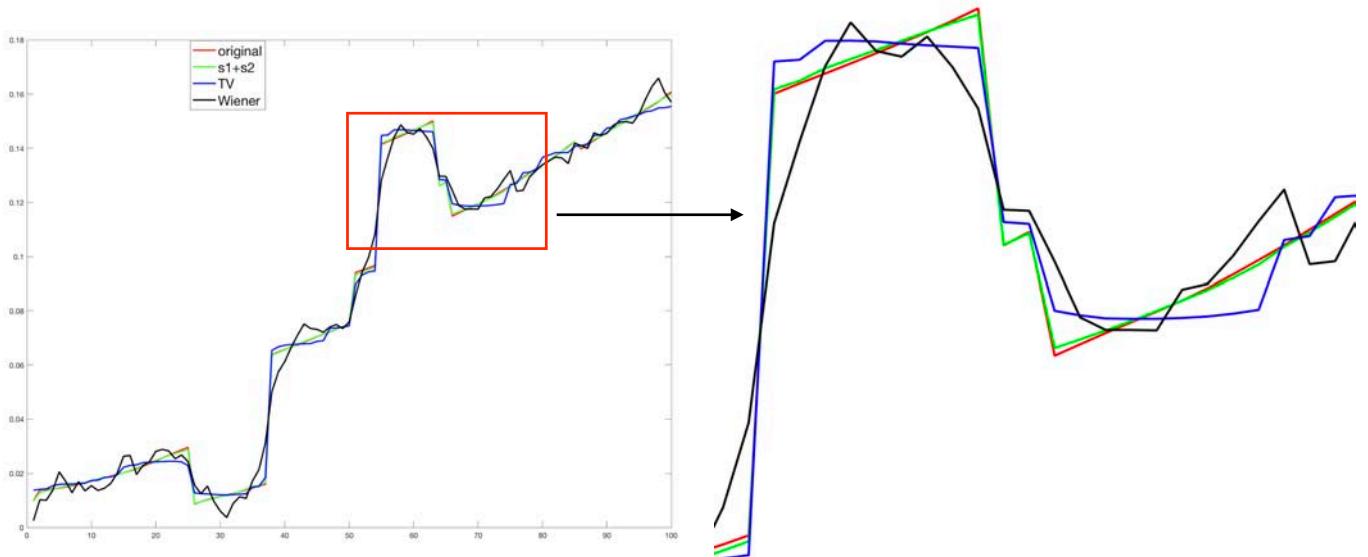
$$\text{Hybrid: } \min_{\mathbf{s}_1, \mathbf{s}_2} \|\mathbf{y} - \mathbf{H}(\mathbf{s}_1 + \mathbf{s}_2)\|_2^2 + \lambda_1 \|\mathbf{D}\mathbf{s}_1\|_1 + \lambda_2 \|\mathbf{D}^2\mathbf{s}_2\|_2^2$$

$$\text{TV: } \min_{\mathbf{s}} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \lambda \|\mathbf{D}\mathbf{s}\|_1$$

$$\text{Wiener: } \min_{\mathbf{s}} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \lambda \|\mathbf{D}^2\mathbf{s}\|_2^2$$

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## Example 1

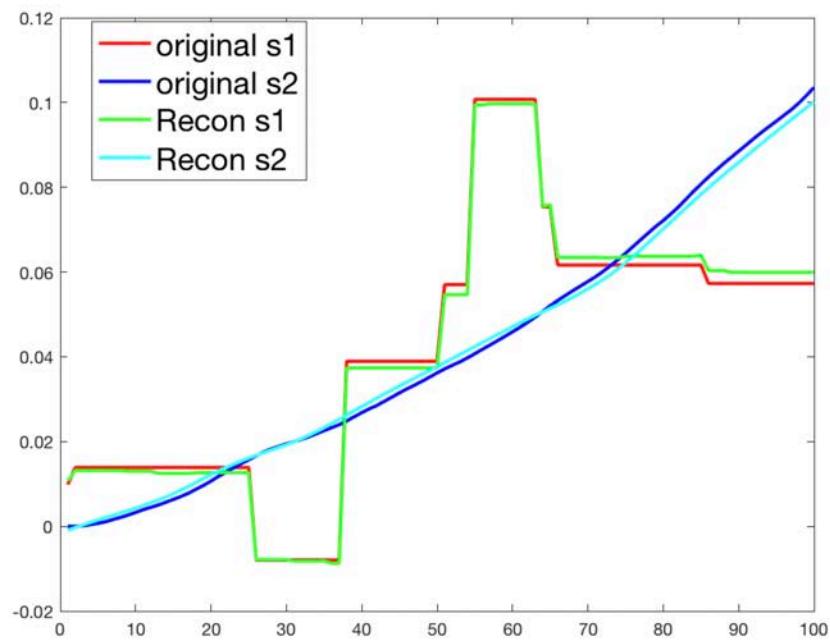


Number of measurements: M = 31

Number of basis functions: K=100

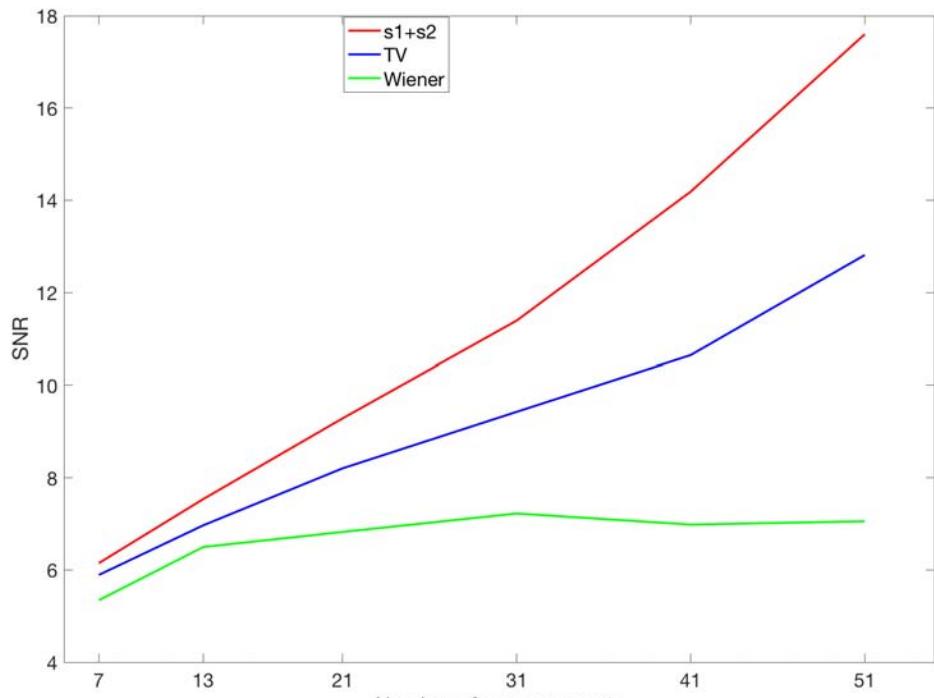
32

## Example 1 - Unmixed components



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## Comparison



Average performance over 20 signals

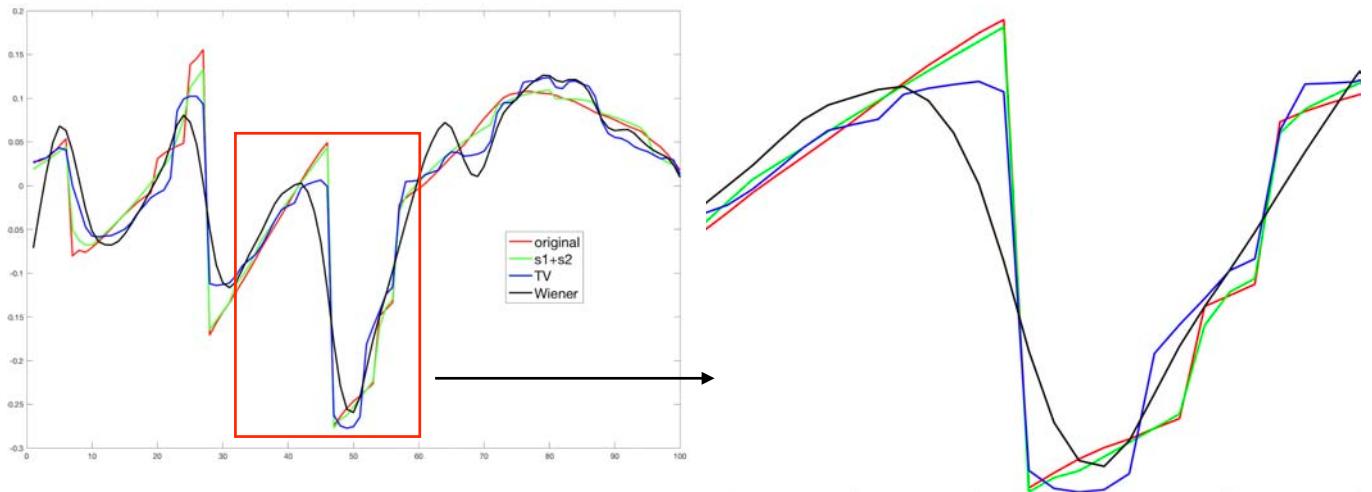
34

## Example 2

$$s = s_1 + s_2$$

$$L_1 = D, \quad w_1: \text{impulsive noise}$$

$$L_2 = D^2, \quad w_2: \text{Gaussian noise}$$



Number of measurements:  $M = 31$

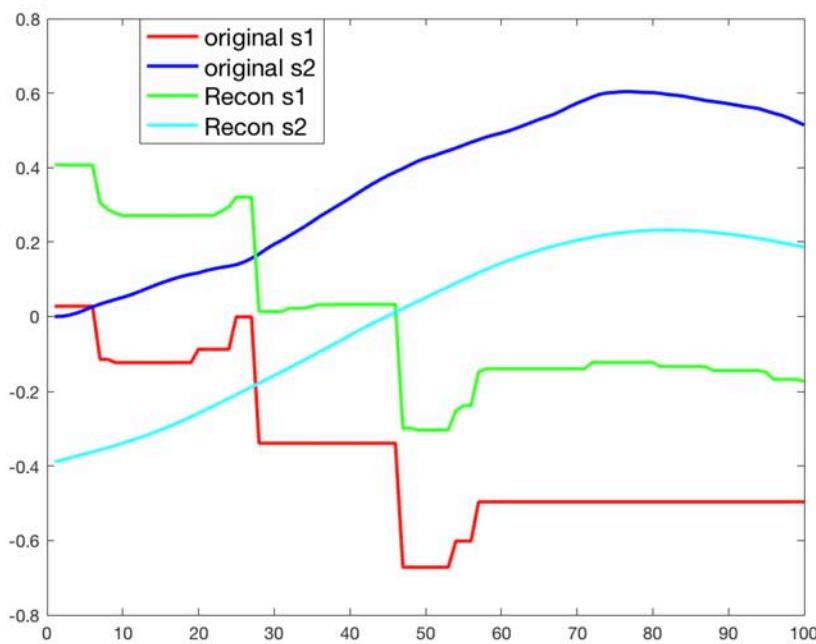
Number of basis functions:  $K=100$

35

## Example 2 - Unmixed components

$$L_1 = D, \quad w_1: \text{impulsive noise}$$

$$L_2 = D^2, \quad w_2: \text{Gaussian noise}$$



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# CONCLUSION

- Unifying continuous-domain stochastic model
  - Backward compatibility with classical Gaussian theory
  - Operator-based formulation: Lévy-driven SDEs or SPDEs
  - Gaussian vs. **sparse** (generalized Poisson, student, S $\alpha$ S)
- Regularization
  - Sparsification via “operator-like” behavior (whitening)
  - Specific family of id potential functions (typ., non-convex)
- Conceptual framework for sparse signal recovery
  - Principled approach for the development of algorithms
  - **Generalization:** hybrid models
    - link with sparse encoding, dictionary-based methods
- Challenges
  - Model identification / learning (self-tuning)

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- Dr. Masih Nilchian
- Pakshal Bohra
- Thomas Debarre
- ....



and collaborators ...

- Prof. Demetri Psaltis
- Prof. Marco Stampanoni
- Prof. Carlos-Oscar Sorzano
- Dr. Arne Seitz
- ....



- Preprints and demos: <http://bigwww.epfl.ch/>

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# References

## ■ Theory of sparse stochastic processes

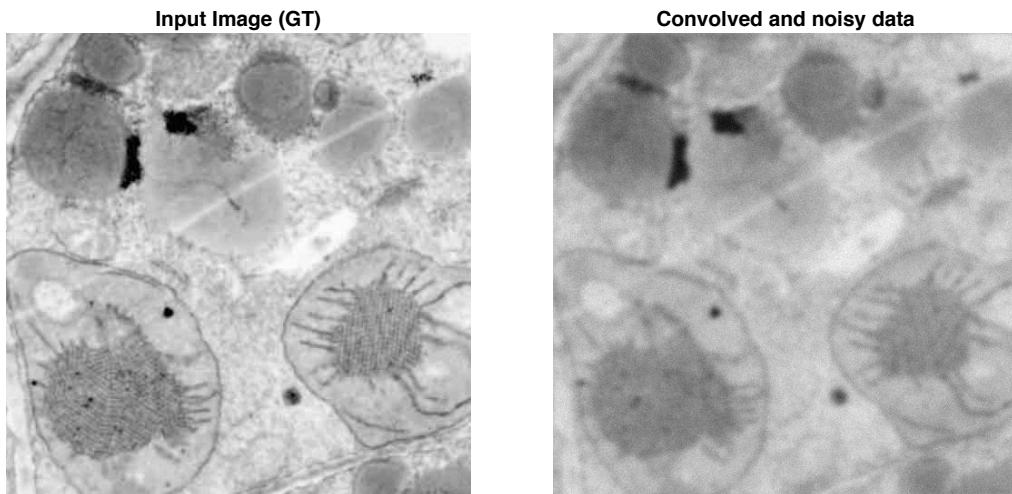
- M. Unser and P. Tafti, **An Introduction to Sparse Stochastic Processes**, Cambridge University Press, 2014; preprint, available at <http://www.sparseprocesses.org>.
- M. Unser, P.D. Tafti, "Stochastic models for sparse and piecewise-smooth signals", *IEEE Trans. Signal Processing*, vol. 59, no. 3, pp. 989-1006, March 2011.
- M. Unser, P. Tafti, and Q. Sun, "A unified formulation of Gaussian vs. sparse stochastic processes—Part I: Continuous-domain theory," *IEEE Trans. Information Theory*, vol. 60, no. 3, pp. 1945-1962, March 2014.

## ■ Algorithms and imaging applications

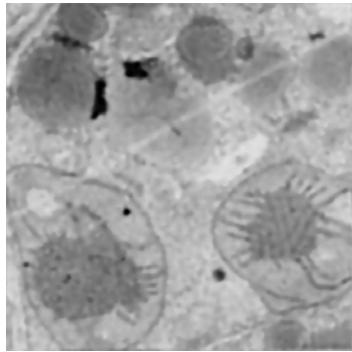
- E. Bostan, U.S. Kamilov, M. Nilchian, M. Unser, "Sparse Stochastic Processes and Discretization of Linear Inverse Problems," *IEEE Trans. Image Processing*, vol. 22, no. 7, pp. 2699-2710, 2013.
- C. Vonesch, M. Unser, "A Fast Multilevel Algorithm for Wavelet-Regularized Image Restoration," *IEEE Trans. Image Processing*, vol. 18, no. 3, pp. 509-523, March 2009.
- M. Nilchian, C. Vonesch, S. Lefkimiatis, P. Modregger, M. Stampanoni, M. Unser, "Constrained Regularized Reconstruction of X-Ray-DPCI Tomograms with Weighted-Norm," *Optics Express*, vol. 21, no. 26, pp. 32340-32348, 2013.
- T. Debarre, J. Fageot , H. Gupta, M. Unser, "B-Spline-Based Exact Discretization of Continuous-Domain Inverse Problems With Generalized TV Regularization", *IEEE Trans. Information Theory*, in press.

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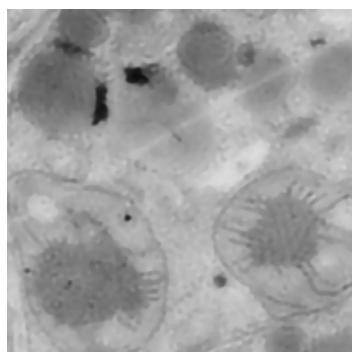
# Ground truth



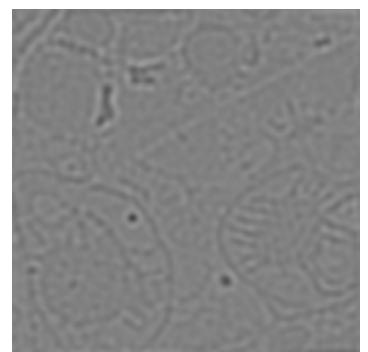
# Hybrid



**SNR = 27.96 dB**



$s_1$  (Total variation)

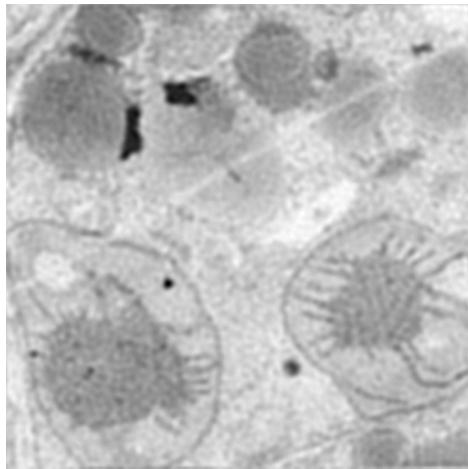


$s_2$  (Sobolev)

$$\arg \min_{\mathbf{c}_1, \mathbf{c}_2 \in \mathbb{R}^N} \|\mathbf{H}(\mathbf{c}_1 + \mathbf{c}_2) - \mathbf{y}\|_2^2 + \lambda \left( \alpha \|\nabla \mathbf{c}_1\|_1 + (1 - \alpha) \|(\Delta + \beta \mathbf{I}) \mathbf{c}_2\|_2^2 \right)$$

$$\lambda = 10, \alpha = 0.001, \beta = 0.1$$

# L2

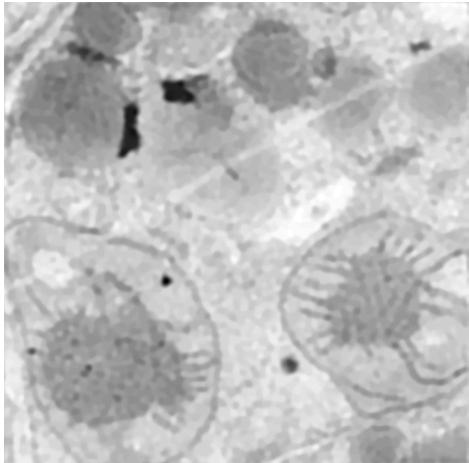


**SNR = 27.87 dB**

$$\arg \min_{\mathbf{c} \in \mathbb{R}^N} \|\mathbf{H}\mathbf{c} - \mathbf{y}\|_2^2 + \lambda \|\Delta \mathbf{c}\|_2^2$$

$$\lambda = 0.2$$

# TV



**SNR = 27.97 dB**

$$\arg \min_{\boldsymbol{c} \in \mathbb{R}^N} \|\mathbf{H}\boldsymbol{c} - \boldsymbol{y}\|_2^2 + \lambda \|\nabla \boldsymbol{c}\|_1$$

$$\lambda=0.002$$