

# **Disentangling respiratory, cardiogenic and vasomotor rhythms from dynamic infrared thermogram signals**

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**Institute of Continuous Media Mechanics, Perm, Russia**

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**Perm State Academy of Medecine, Perm, Russia**

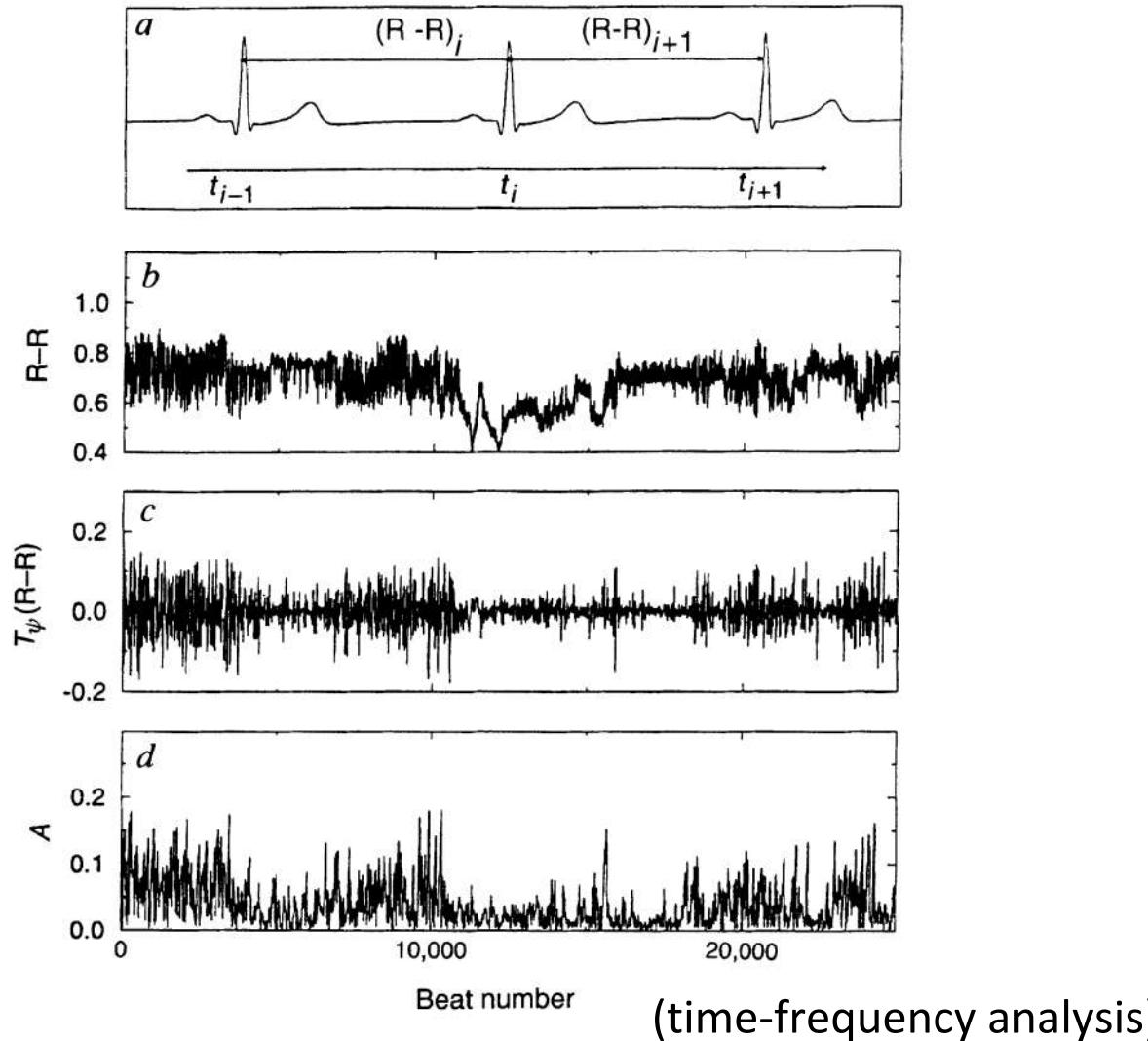
**Olga Gileva**

*E. Gerasimova et al., EPL 104 (2013) 68011*

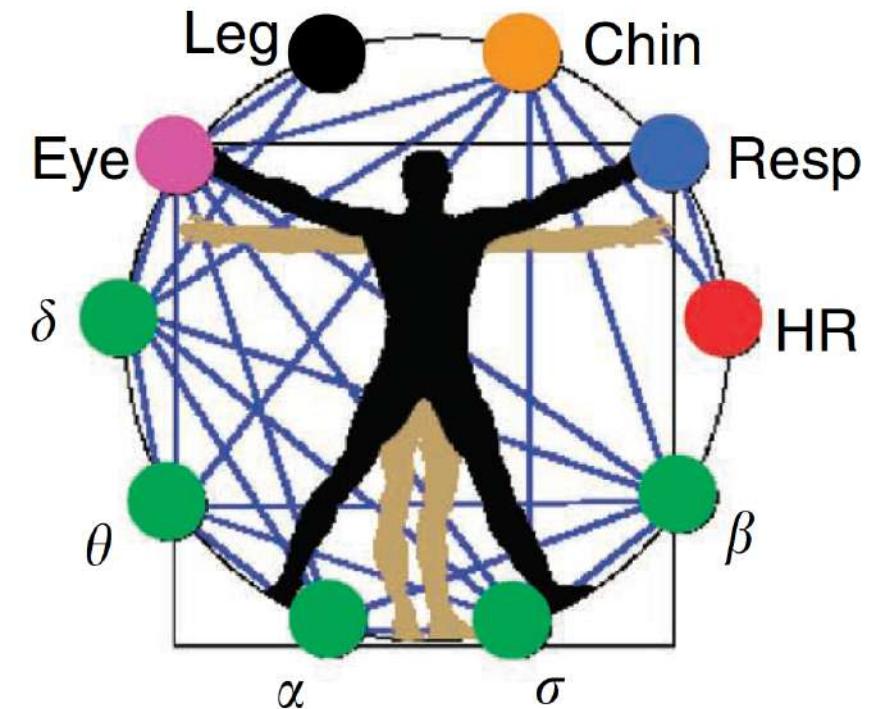
*E. Gerasimova et al., Frontiers in Physiology 5 (2014) 176*

# Physiological networks : the inter-node dynamics complexity is the issue

*Scaling behavior of heartbeat intervals*  
Ivanov et al. Nature **1996**



**Network Physiology** ->  
Network Topology <-> Physiological Function  
Bashan Nature Communications **2012**

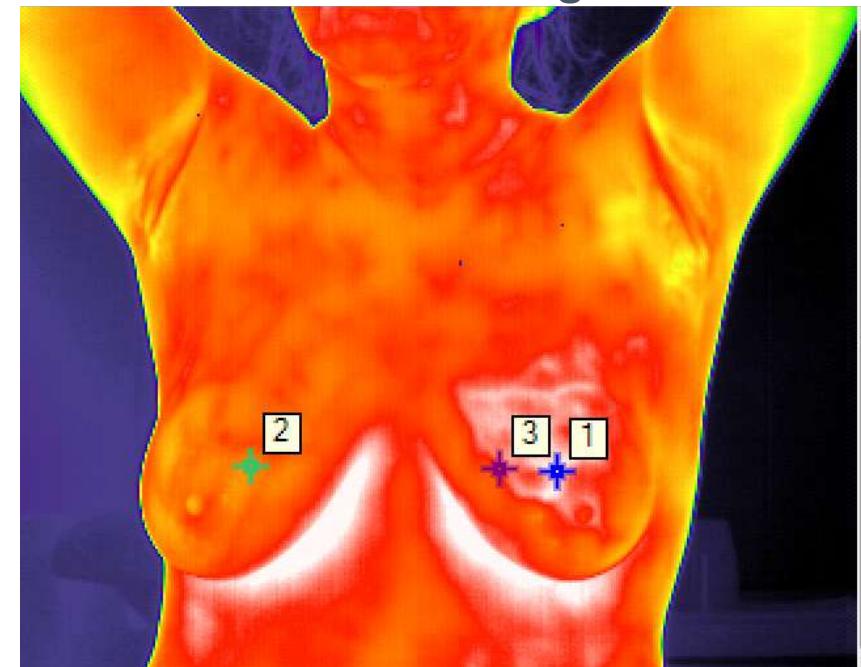


Infrared camera

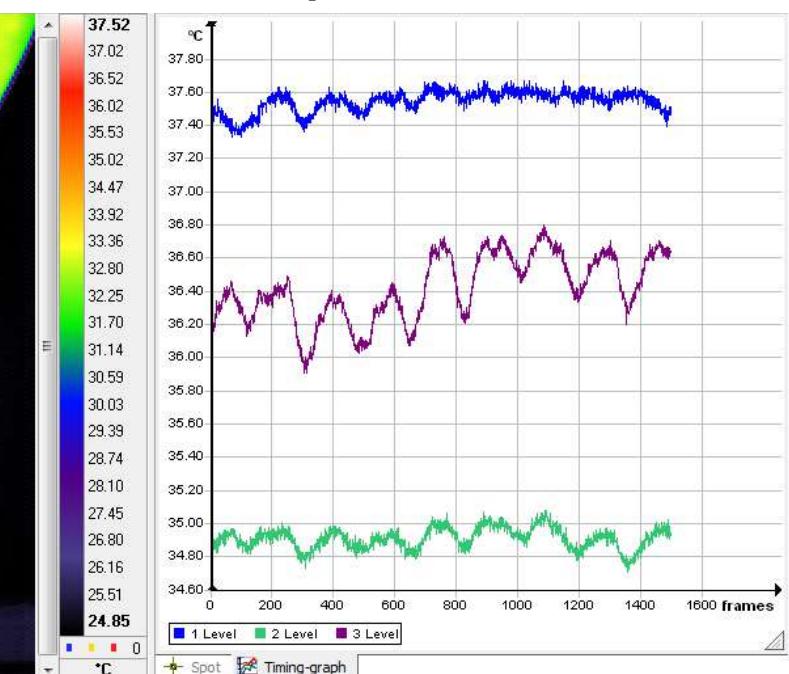


IR thermography to assist cancer diagnosis

Breast thermogram



Temperature time series



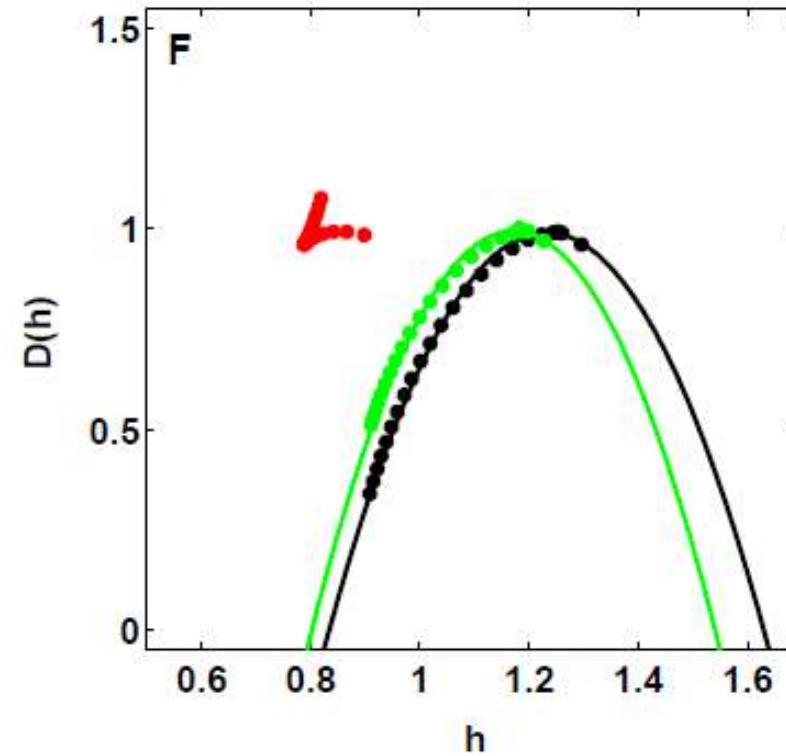
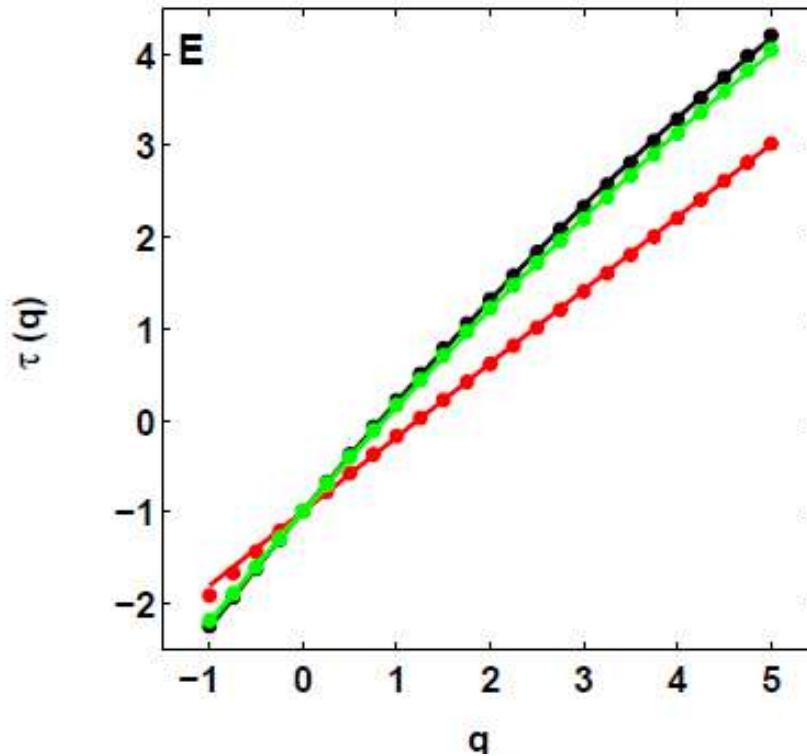
..... -> IR thermography video film

## PLAN OF THE PRESENTATION

- Characterization of the physiological noise of thermogram signals
  - singularity spectra computation based on the wavelet modulus maxima method in both healthy and cancer cases (local temperature averaged on 8x8 pixel squares)
- Disentangling respiratory, cardiogenic rhythms from thermogram signals
  - Respiratory and cardiogenic functions impact on both the spatial position and temperature
  - Time-frequency analysis based on temporal temperature signals averaged over the whole breast
  - Translation and Affine algorithm to extract these displacements
  - Comparing the time-frequency analysis before and after the correction
  - Disentangling respiratory from cardiogenic rhythms

# Multifractal spectra of cumulative IR temperature time series

Average over 8x8 pixel<sup>2</sup>



$$\tau(q) = -c_0 + c_1 q - c_2 q^2 / 2$$
$$D(h) = c_0 - (h - c_1)^2 / 2c_2$$

Cancer

$[c_0, c_1, c_2] = [0.99, 0.81, 0.0044]$

Opposite

$[c_0, c_1, c_2] = [0.99, 1.23, 0.080]$

Healthy

$[c_0, c_1, c_2] = [0.99, 1.171, 0.069]$

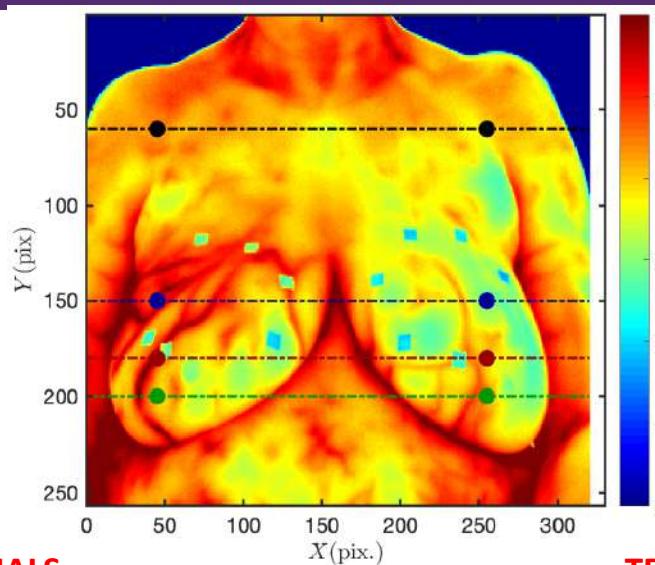
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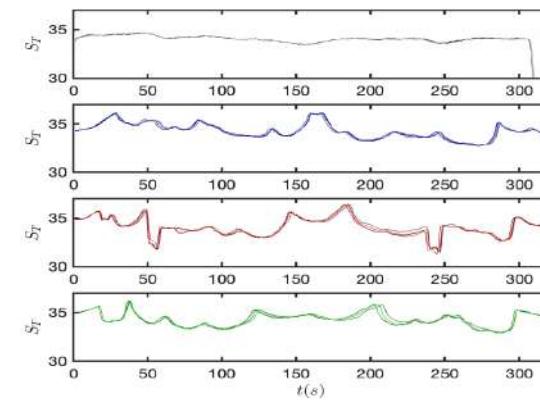
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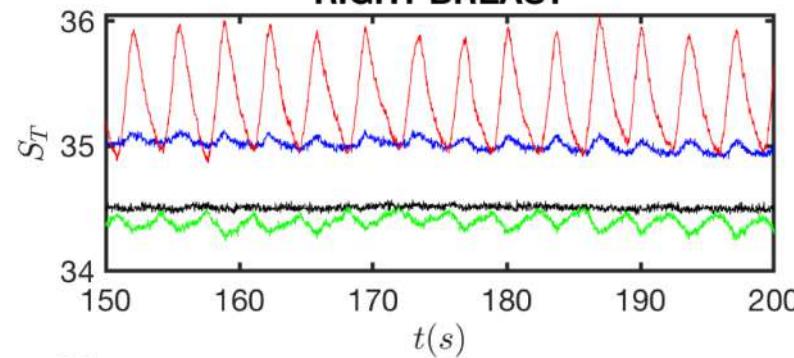
Respiratory and cardiogenic functions impact both the spatial tissue position and skin temperature



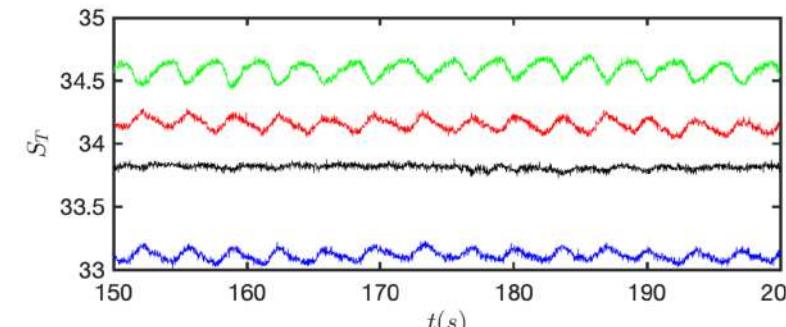
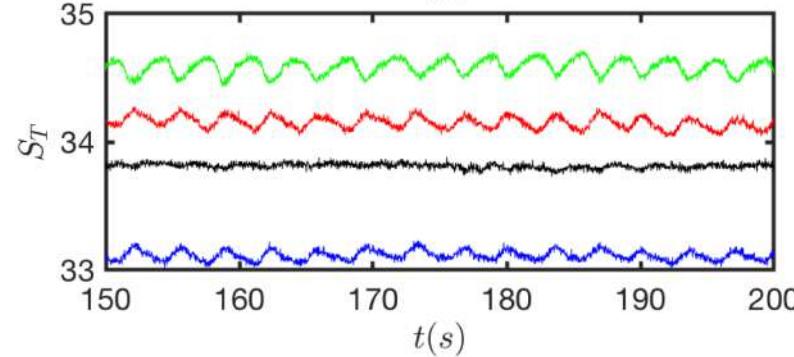
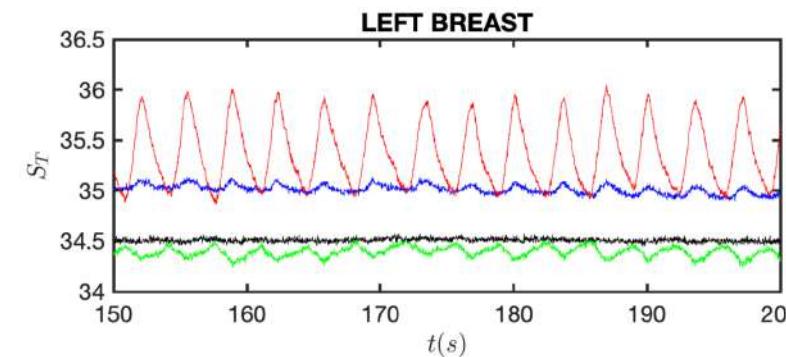
HORIZONTAL SECTIONS



TEMPERATURE SIGNALS  
RIGHT BREAST



TEMPERATURE SIGNALS



# Wavelet transform for time-frequency analysis of rhythmic signals

$$\mathcal{W}_\psi[s](a, t; p) = \int_{-\infty}^{+\infty} s(t') a^{-\frac{1}{p}} \bar{\psi}\left(\frac{t' - t}{a}\right) dt'$$

$\psi$  Wavelet function (in time variable)

(the bar corresponds to the complex conjugate)

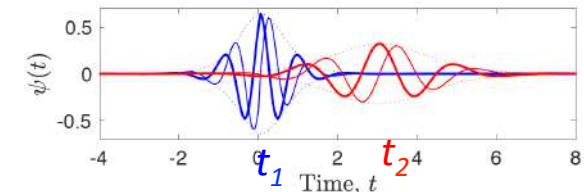
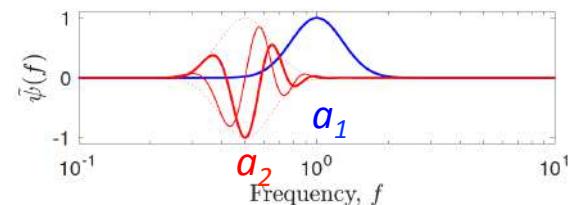
$t$  translation parameter

$a$  scale parameter ( $a = f_0/f$ )

$p$  normalization exponent

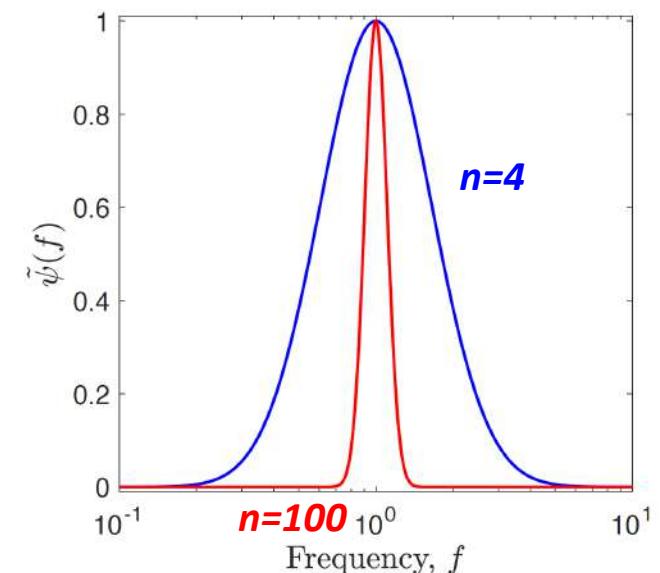
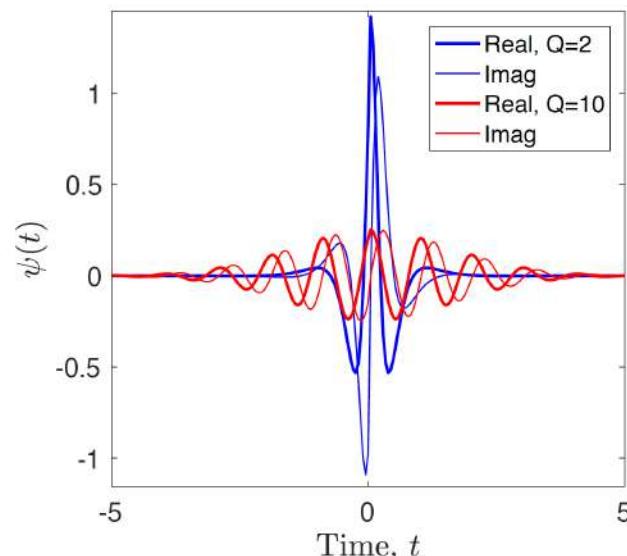
$Q = (n\gamma)^{1/2}$  quality factor

The larger  $Q$ , the sharper the wavelet  
in frequency domain

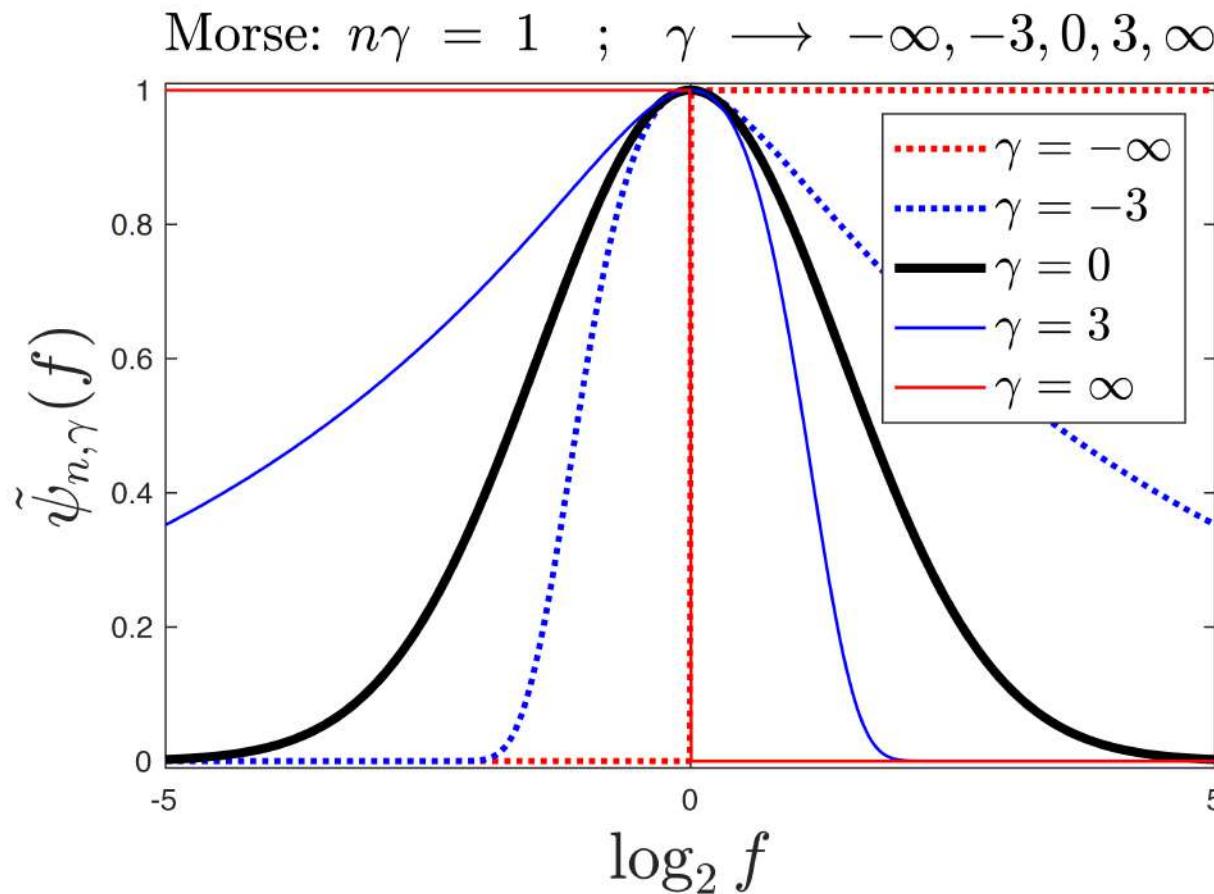


Morse wavelet

$$\tilde{\psi}_{n,\gamma}(f) \propto f^n e^{-f^\gamma} \quad \forall f > 0 \quad ; \quad 0 \text{ if } f \leq 0$$



# Wavelet transform for time-frequency analysis of rhythmic signals



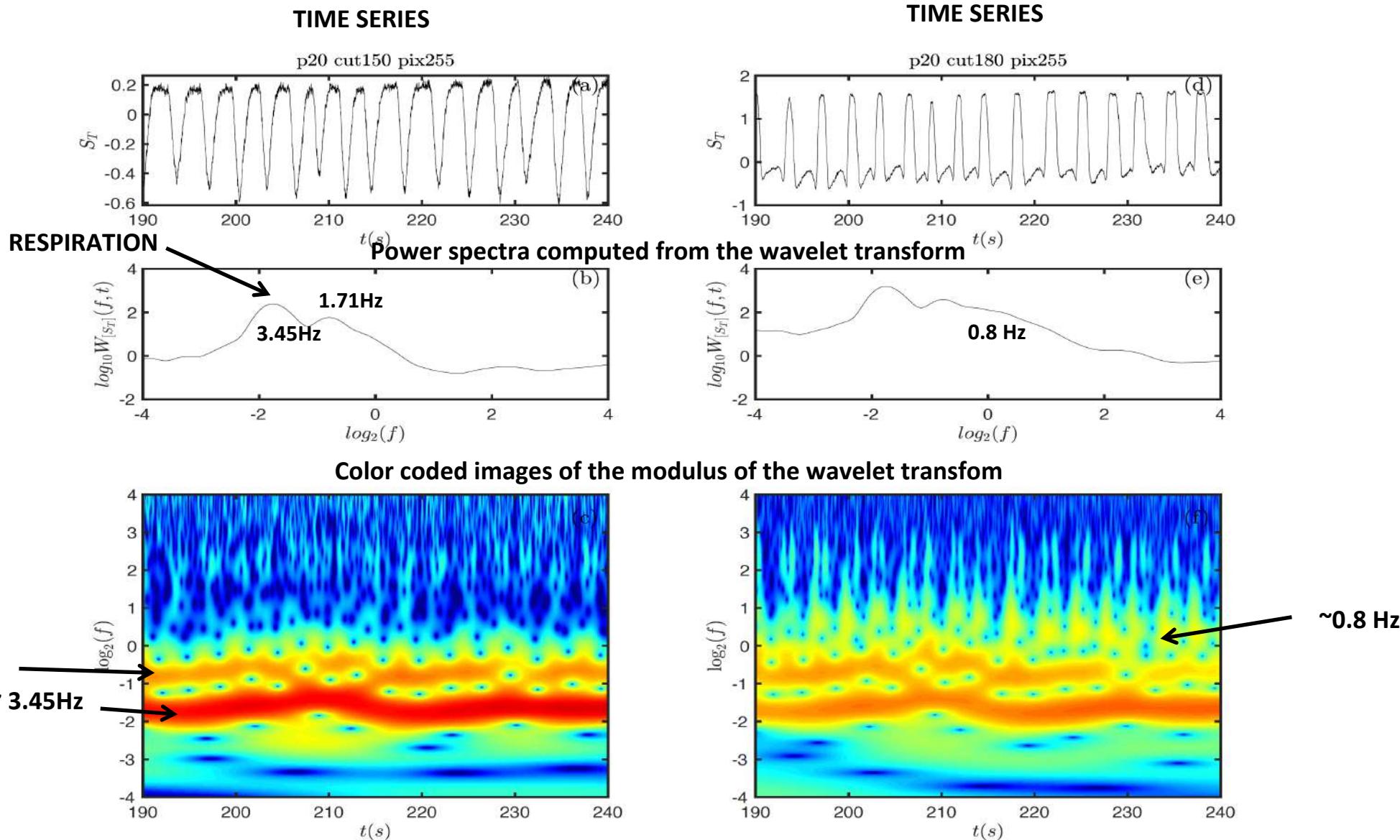
Log-normal Morse wavelet:  $\gamma = 0, n\gamma = 1$

$$\tilde{\psi}_Q(f'/f) = e^{-\frac{1}{2}(Q \log f'/f)^2}$$

This wavelet is symmetric in frequency space  
It is parametrized by the quality factor Q

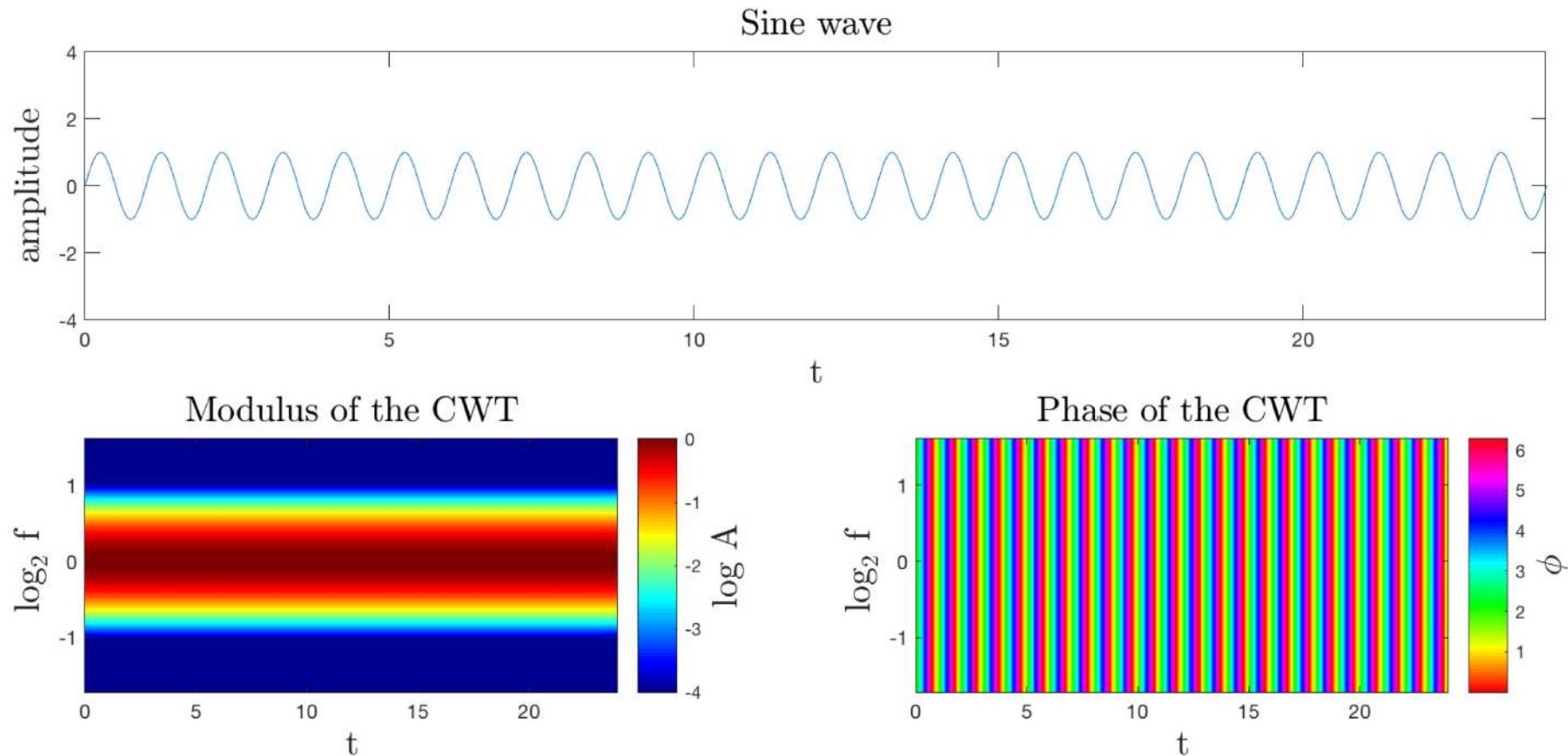
# Wavelet transform for time-frequency analysis of rhythmic signals

Wavelet:  
Morse function  
 $n=32$ ,  $\Upsilon=1$   
 $p=1$



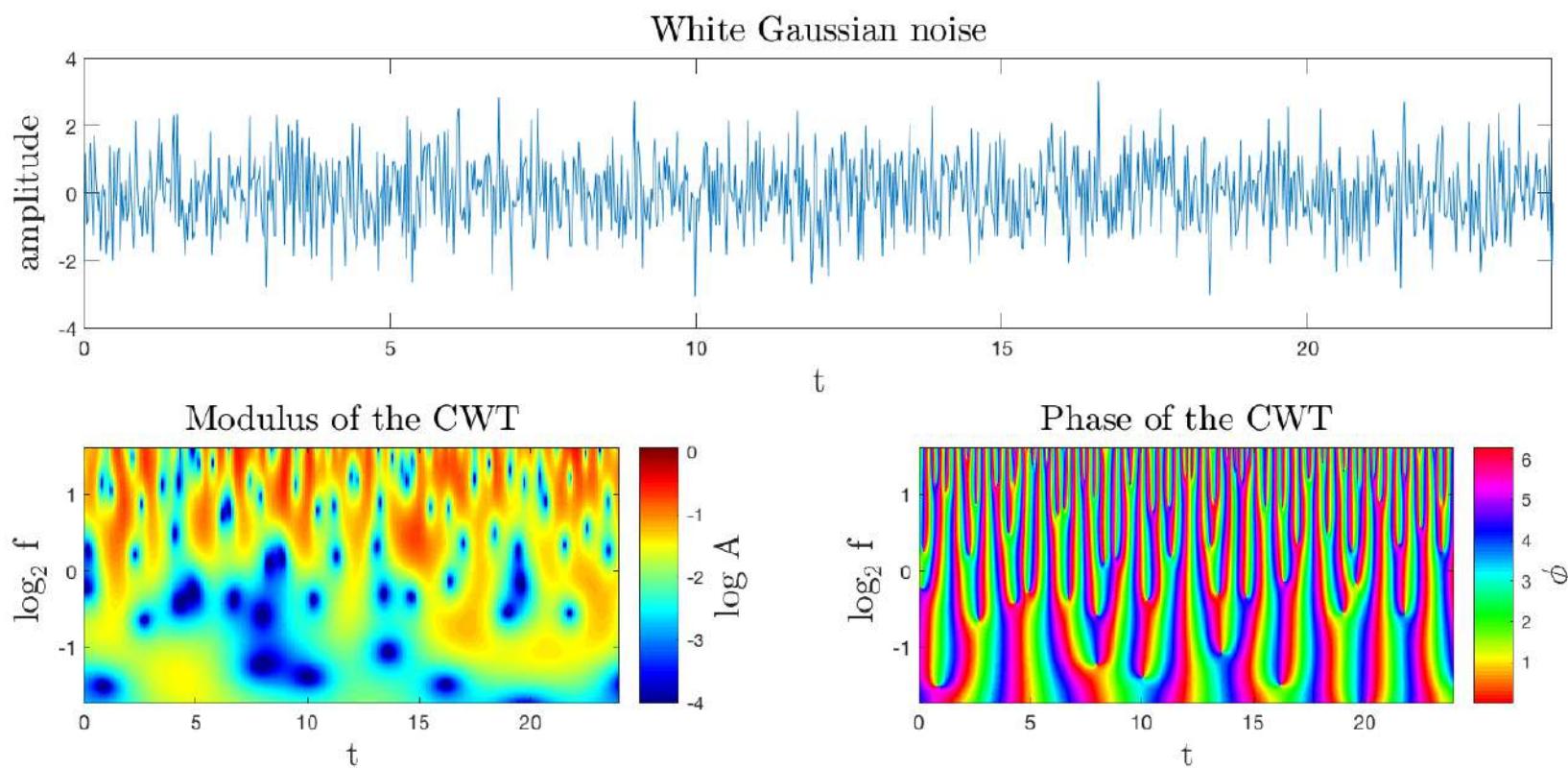
# Wavelet transform analysis of model signals

## PERIODIC SIGNAL (pure sinus)



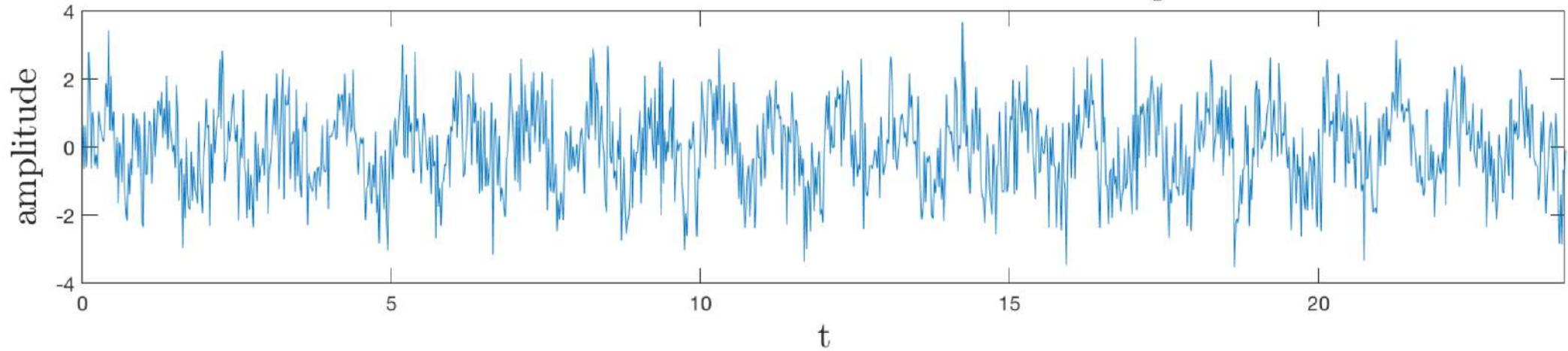
# Wavelet transform analysis of model signals

## RANDOM SIGNAL (no rhythms)

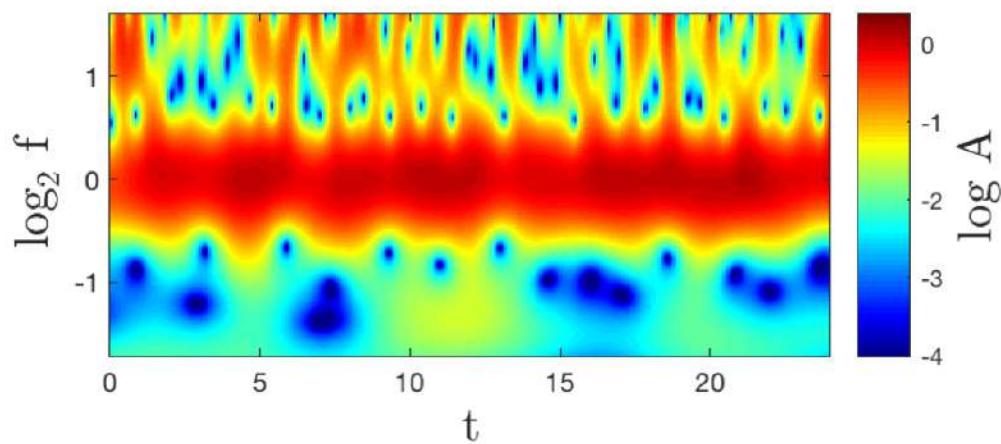


# Wavelet transform analysis of model signals

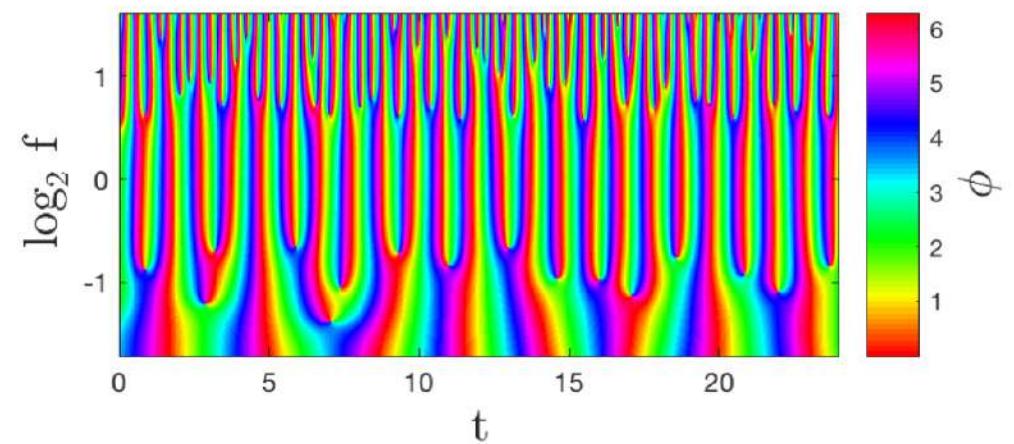
Sine wave + white Gaussian noise with same amplitude



Modulus of the CWT

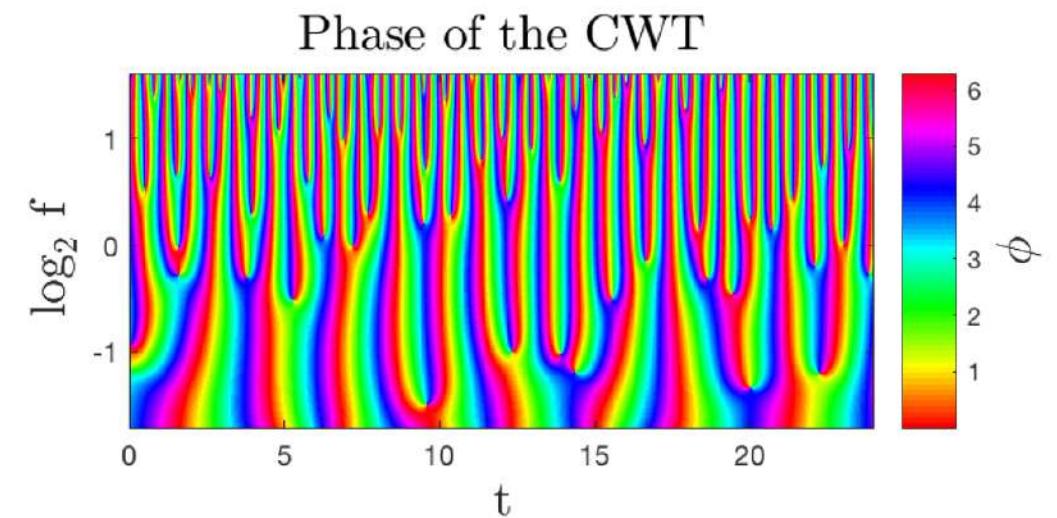
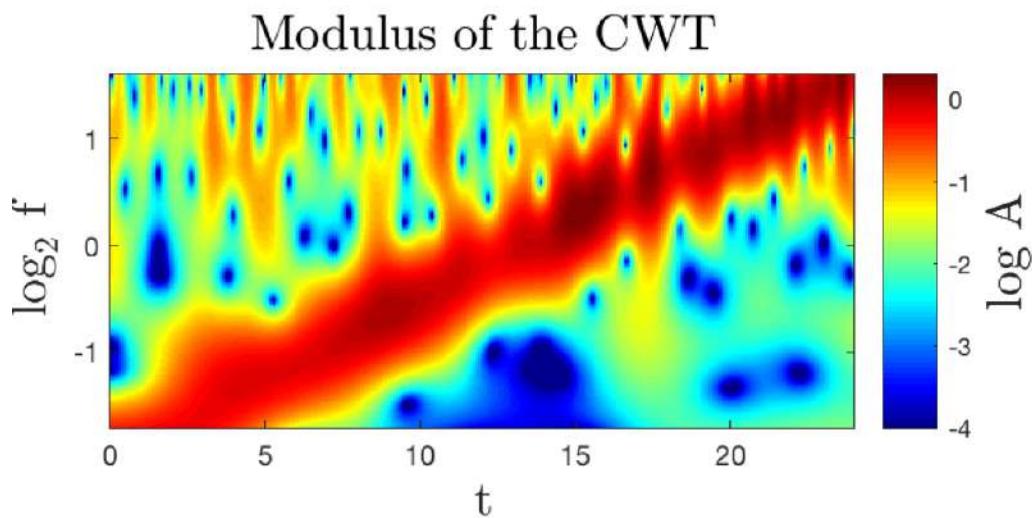
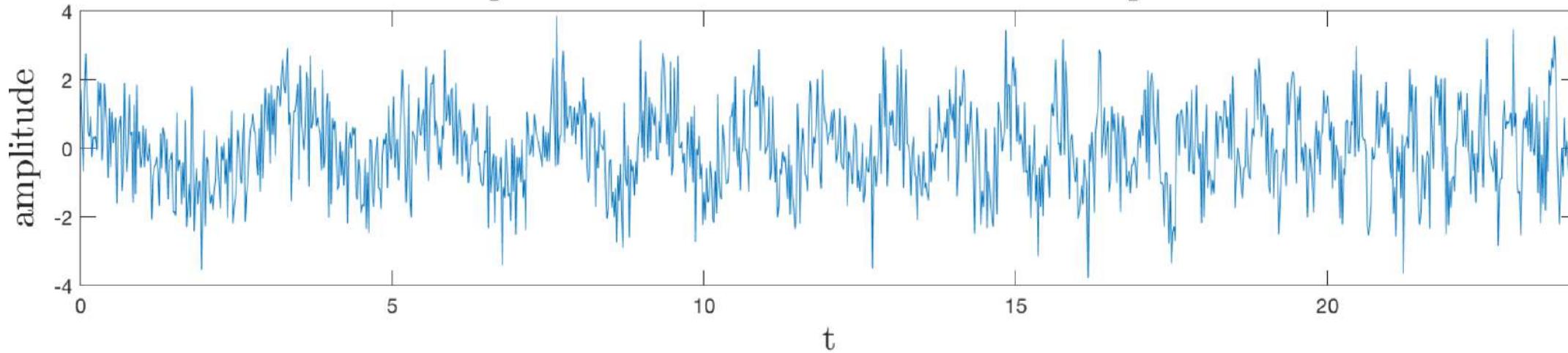


Phase of the CWT



# Wavelet transform analysis of model signals

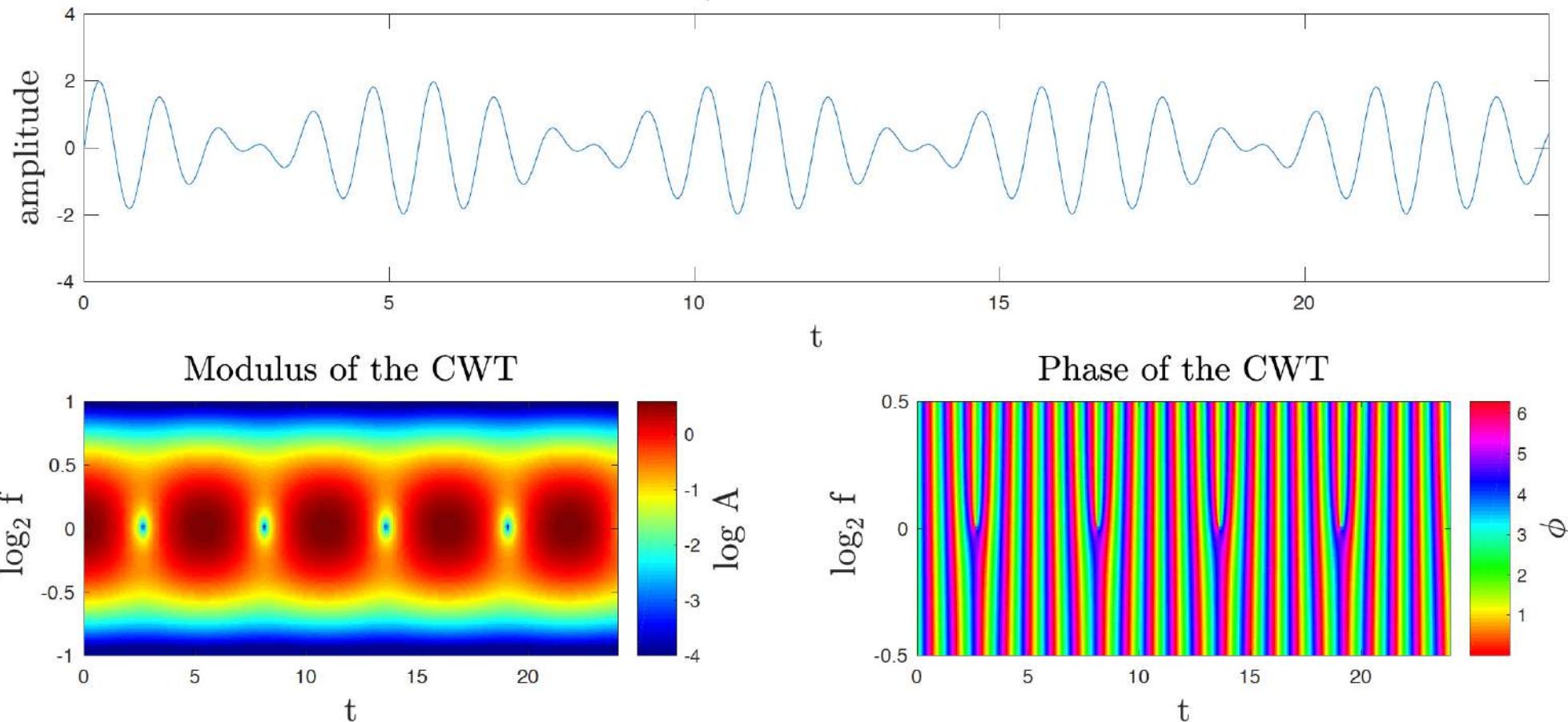
Chirp + white Gaussian noise with same amplitude



# Wavelet transform analysis of model signals: frequency duets

$$S(t) = \sin(ft) + \sin((f+\delta f)t)$$

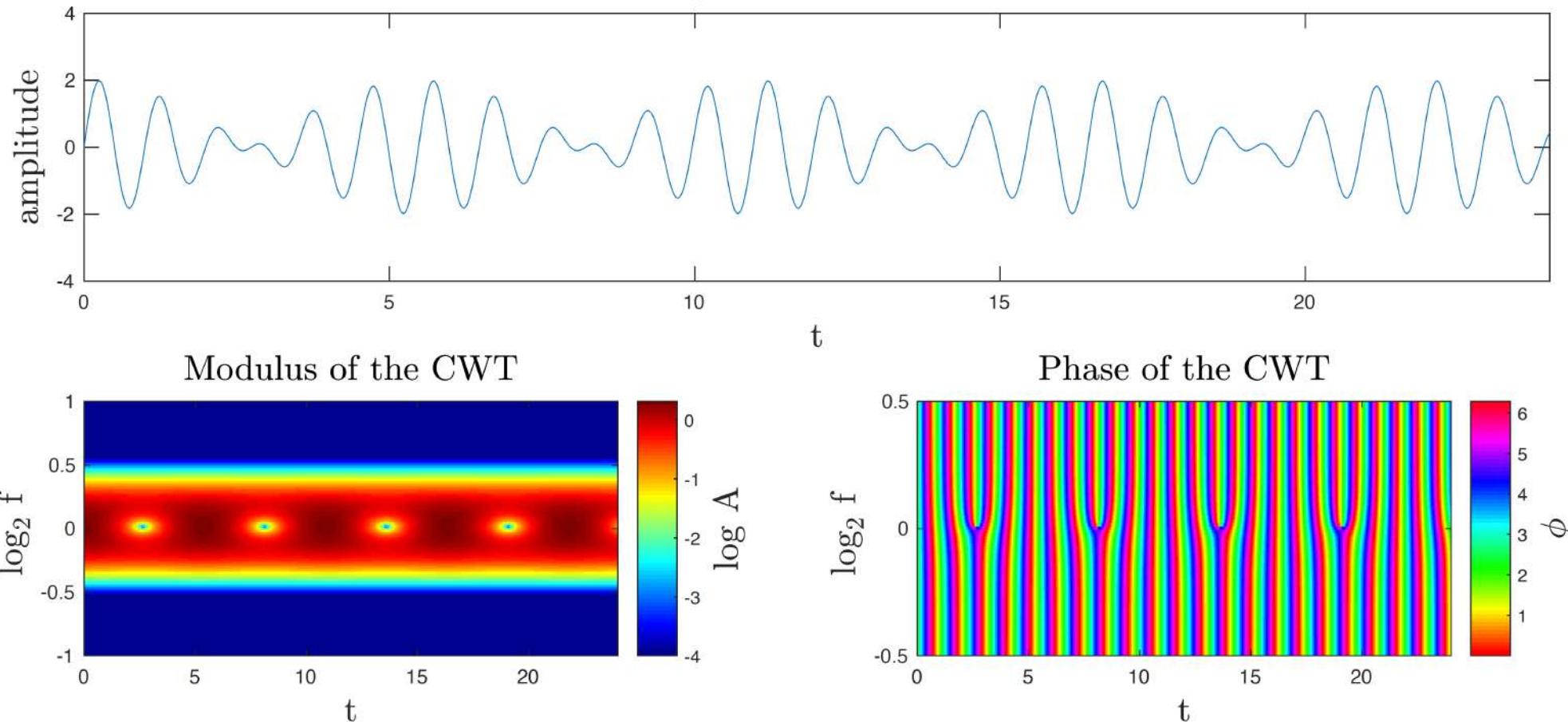
Frequency duet: ratio=1.2, Q=5



# Wavelet transform analysis of model signals: frequency duets

$$S(t) = \sin(ft) + \sin((f+\delta f)t)$$

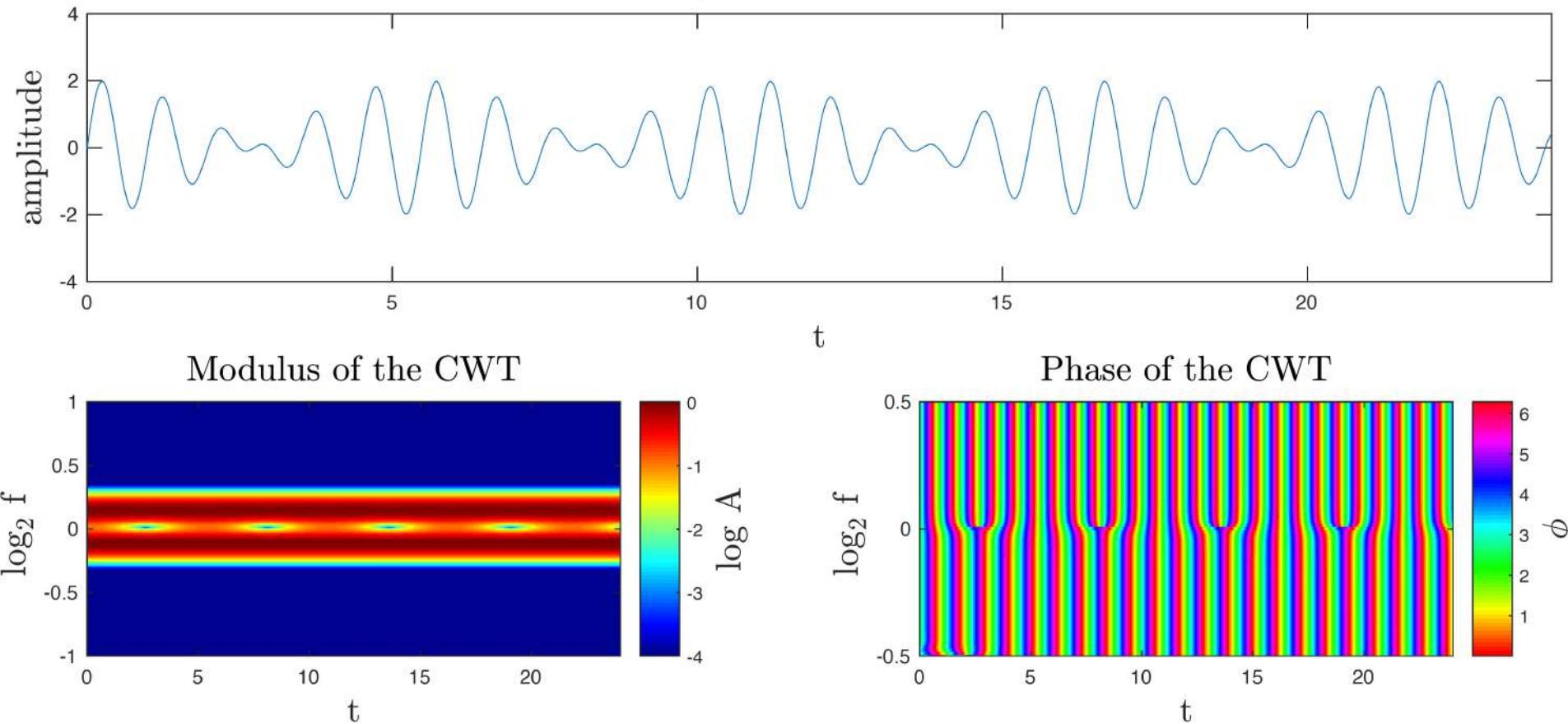
Frequency duet: ratio=1.2, Q=10



# Wavelet transform analysis of model signals: frequency duets

$$S(t) = \sin(ft) + \sin((f+\delta f)t)$$

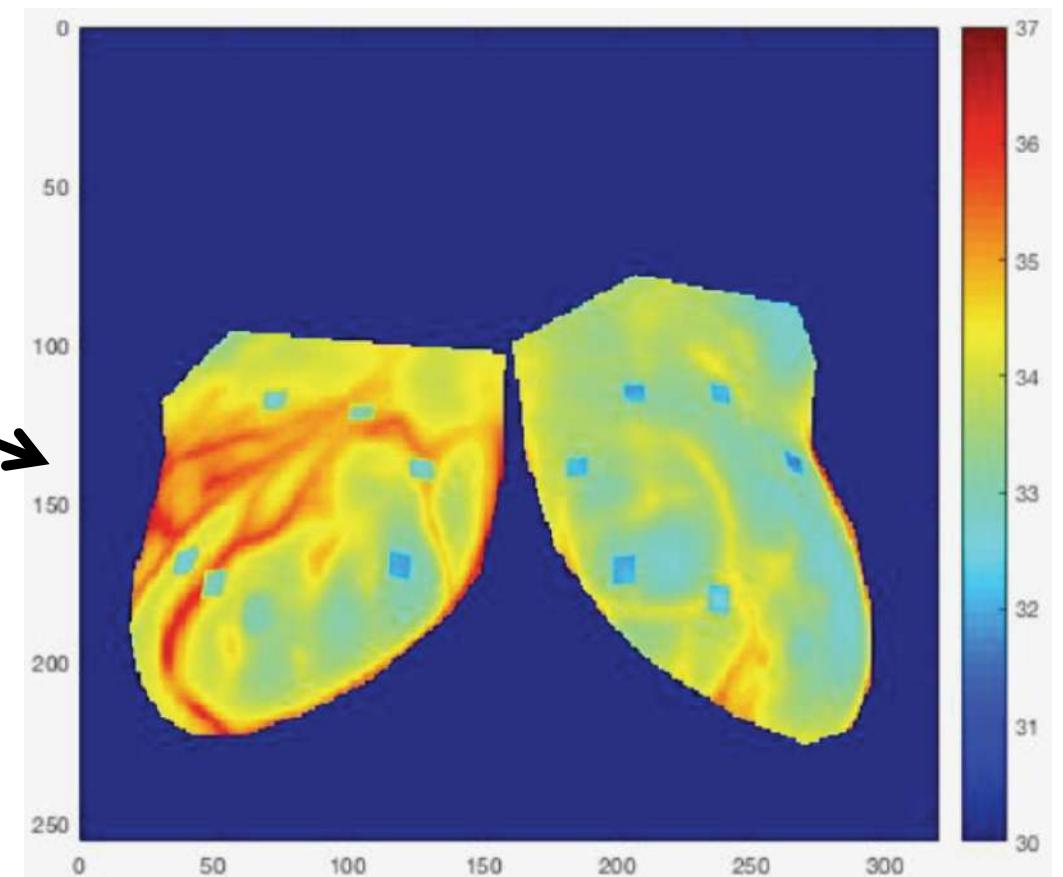
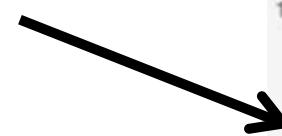
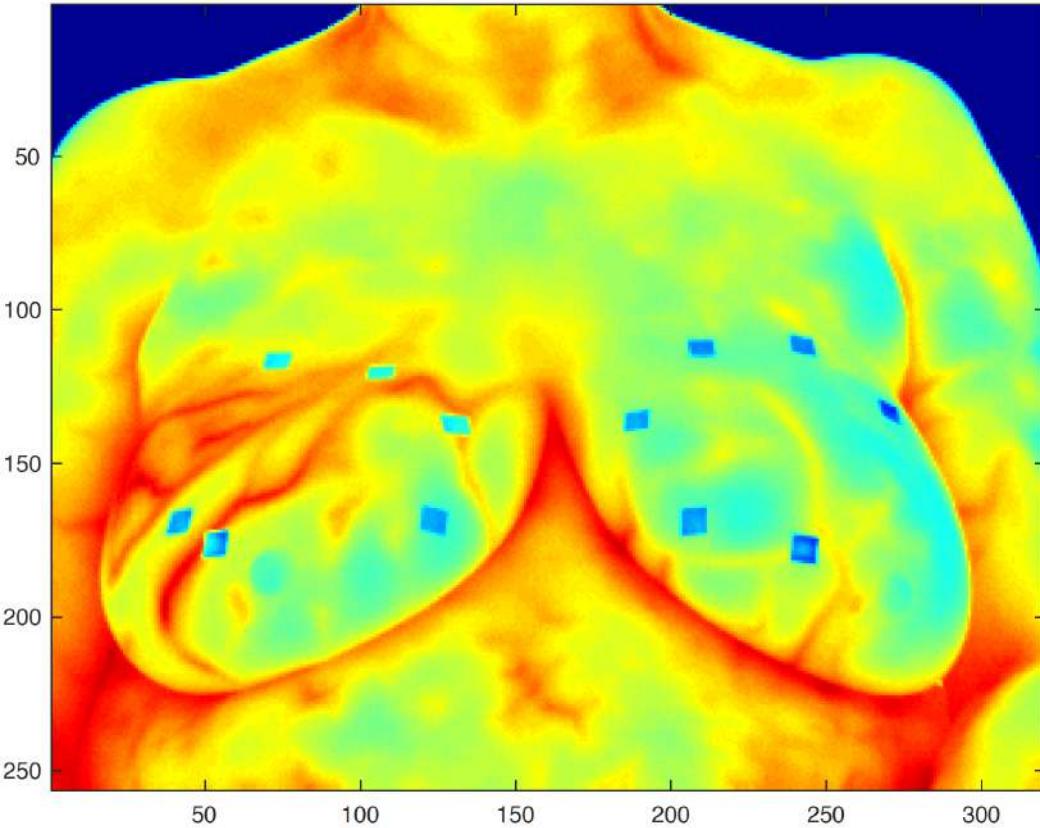
Frequency duet: ratio=1.2, Q=20



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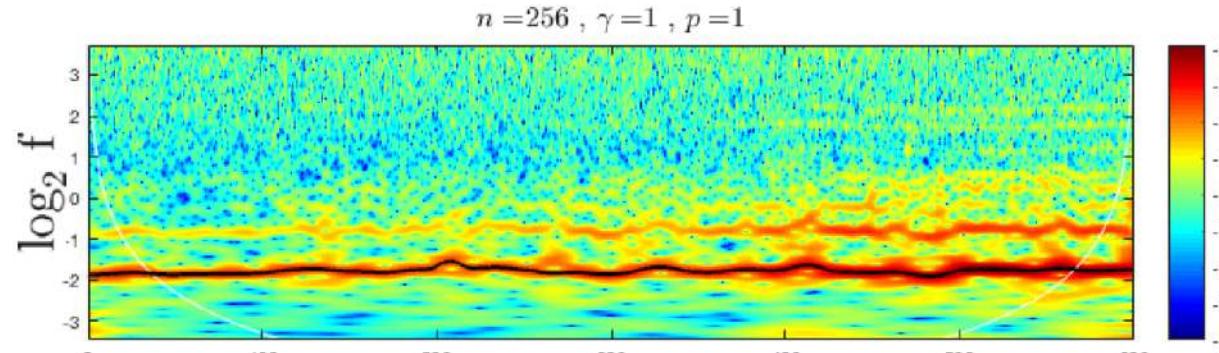
# Global selection of the two breasts (R – L) with ellipse-like shapes



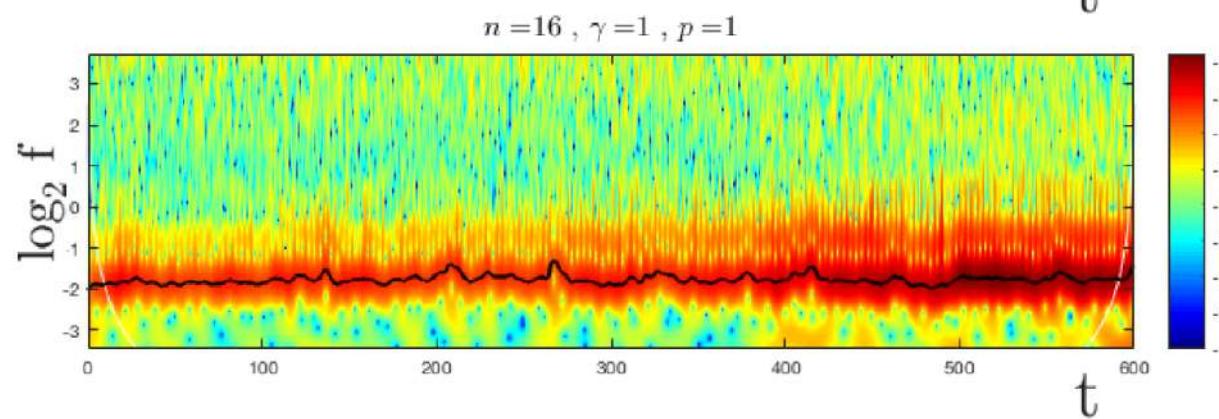
# Influence of the quality factor Q on the detection of the rhythms

$Q = (n\gamma)^{1/2}$  quality factor

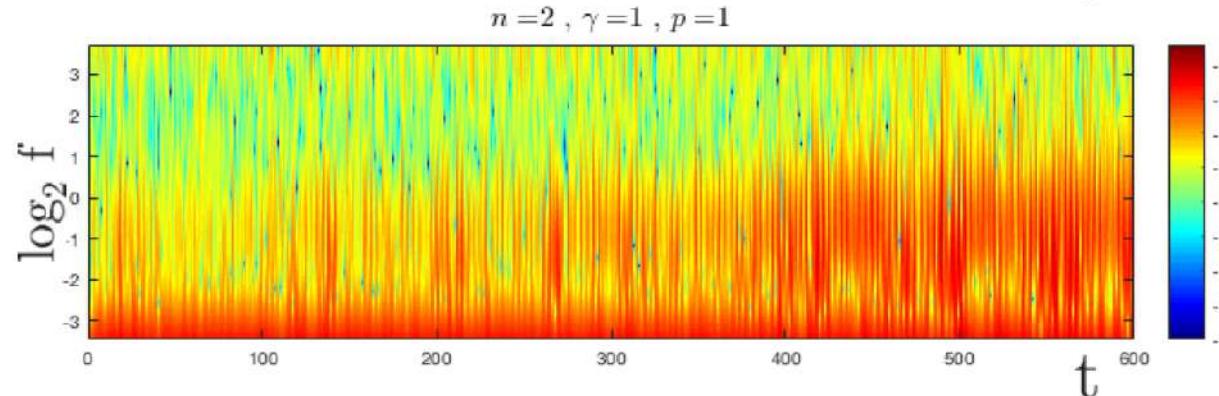
The larger  $Q$ , the sharper the wavelet in frequency domain



High quality factor  
 $Q = 16$



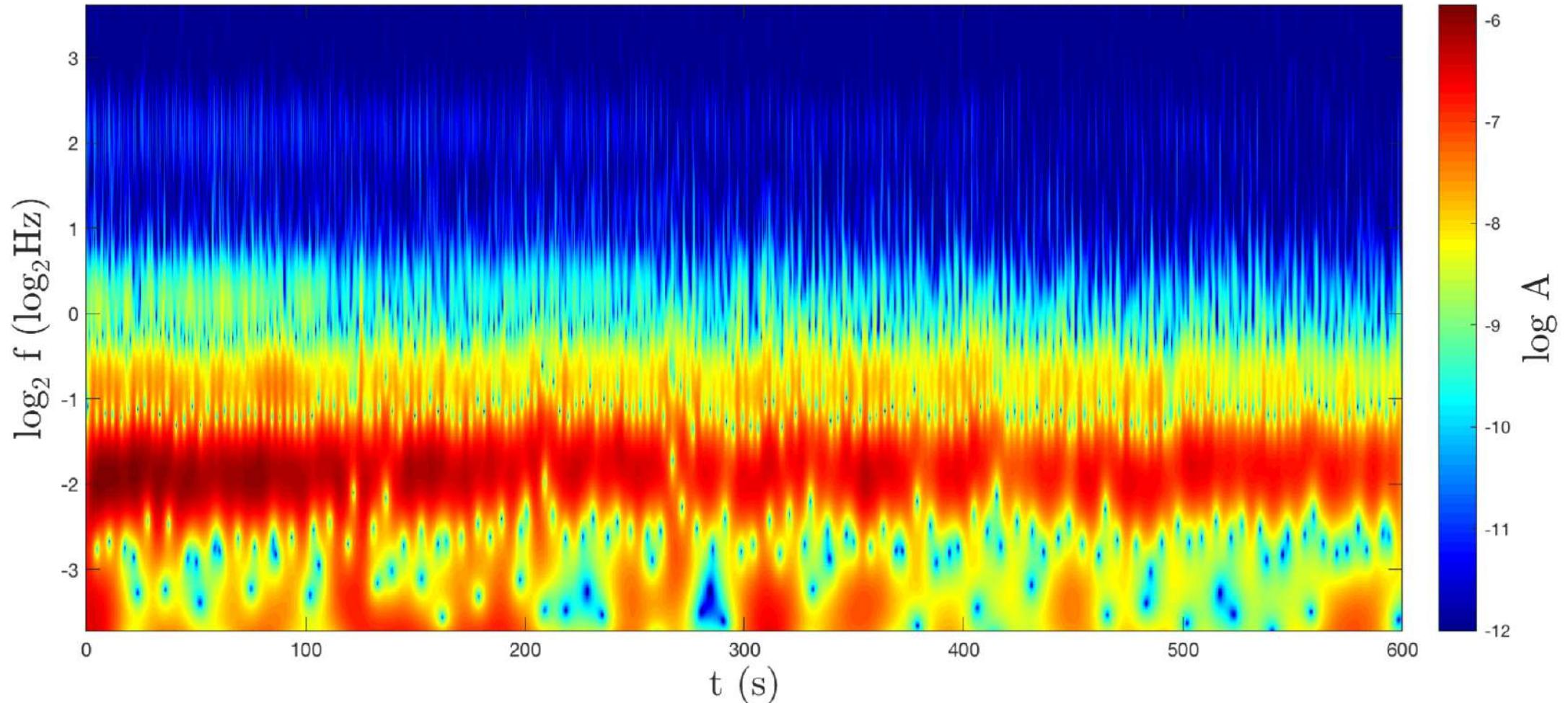
medium quality factor  
 $Q = 4$



Low quality factor  
 $Q = 1.4$

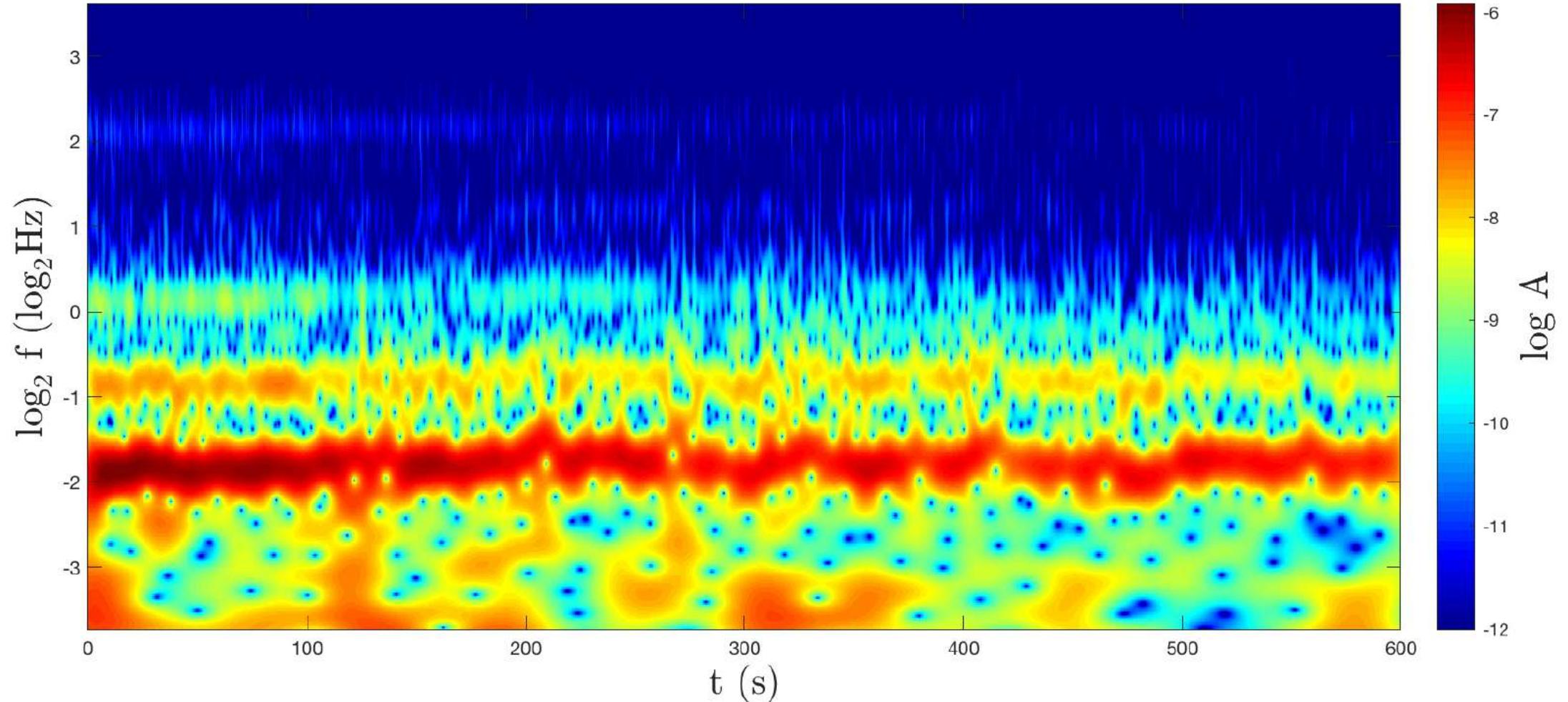
Playing on the wavelet function parameters to reveal both respiratory and cardiac rhythms

Mean of the temperature spatial distribution (p20 left):  $Q = 4$ ,  $p = 2$



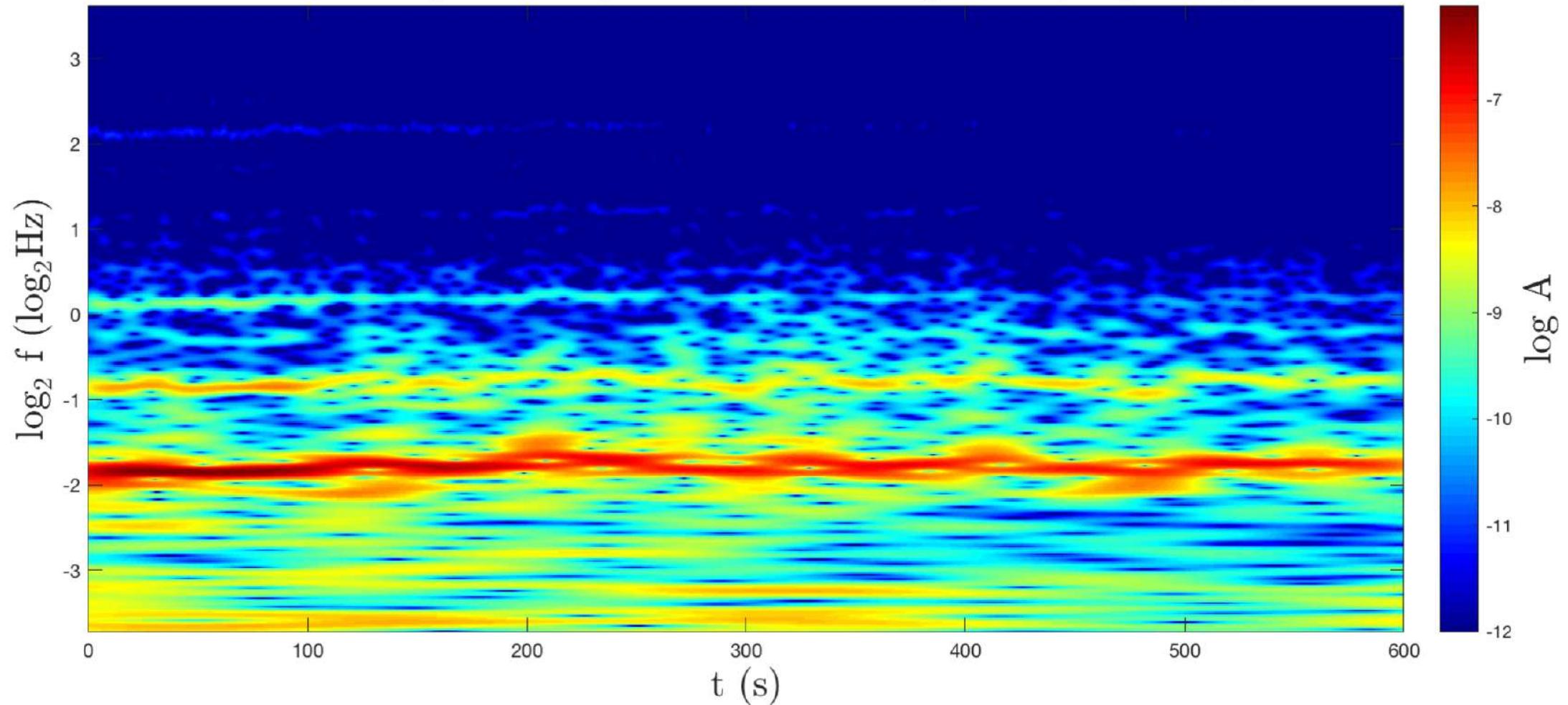
Playing on the wavelet function parameters to reveal both respiratory and cardiac rhythms

Mean of the temperature spatial distribution (p20 left):  $Q = 8$ ,  $p = 2$



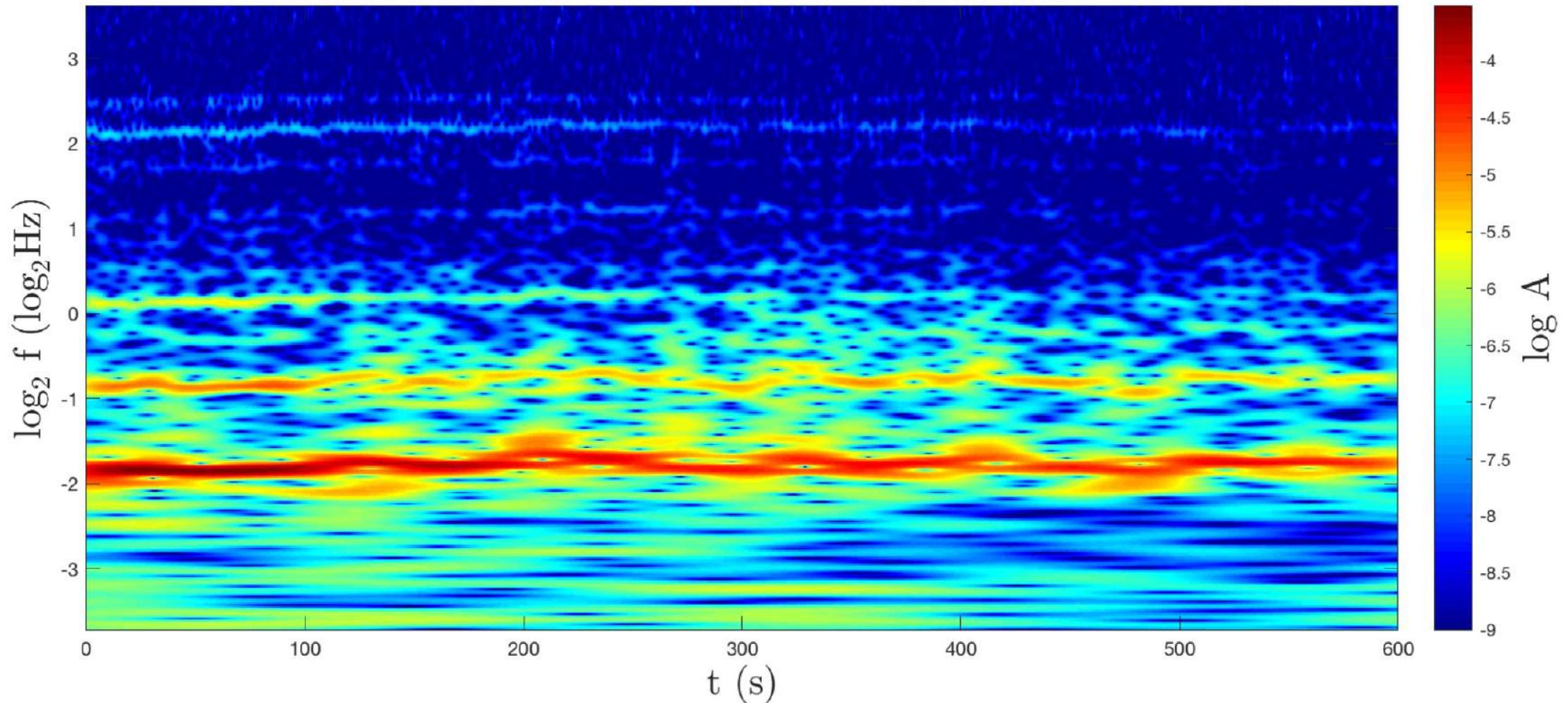
Playing on the wavelet function parameters to reveal both respiratory and cardiac rhythms

Mean of the temperature spatial distribution (p20 left):  $Q = 32$ ,  $p = 2$



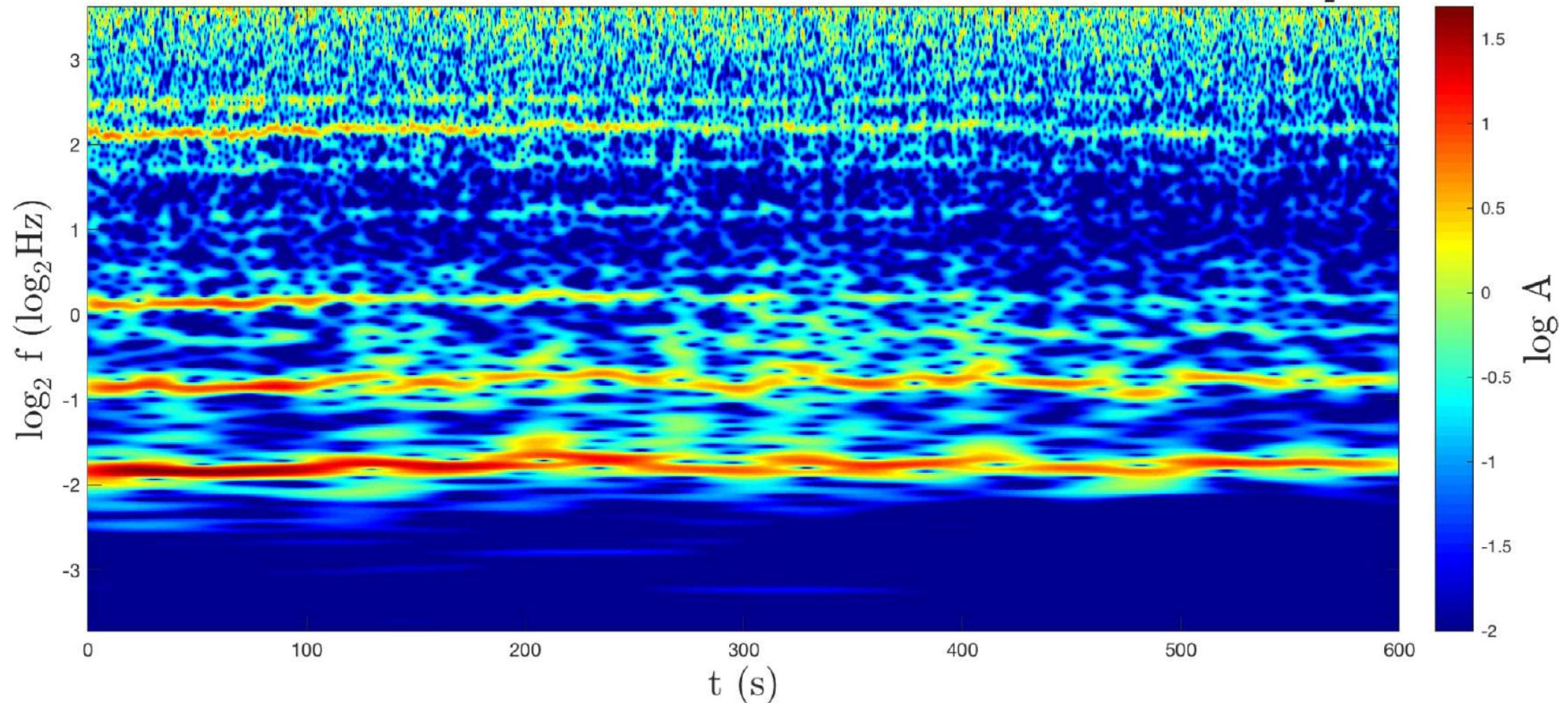
Playing on the wavelet function parameters to reveal both respiratory and cardiac rhythms

Mean of the temperature spatial distribution (p20 left):  $Q = 32$ ,  $p = 1$

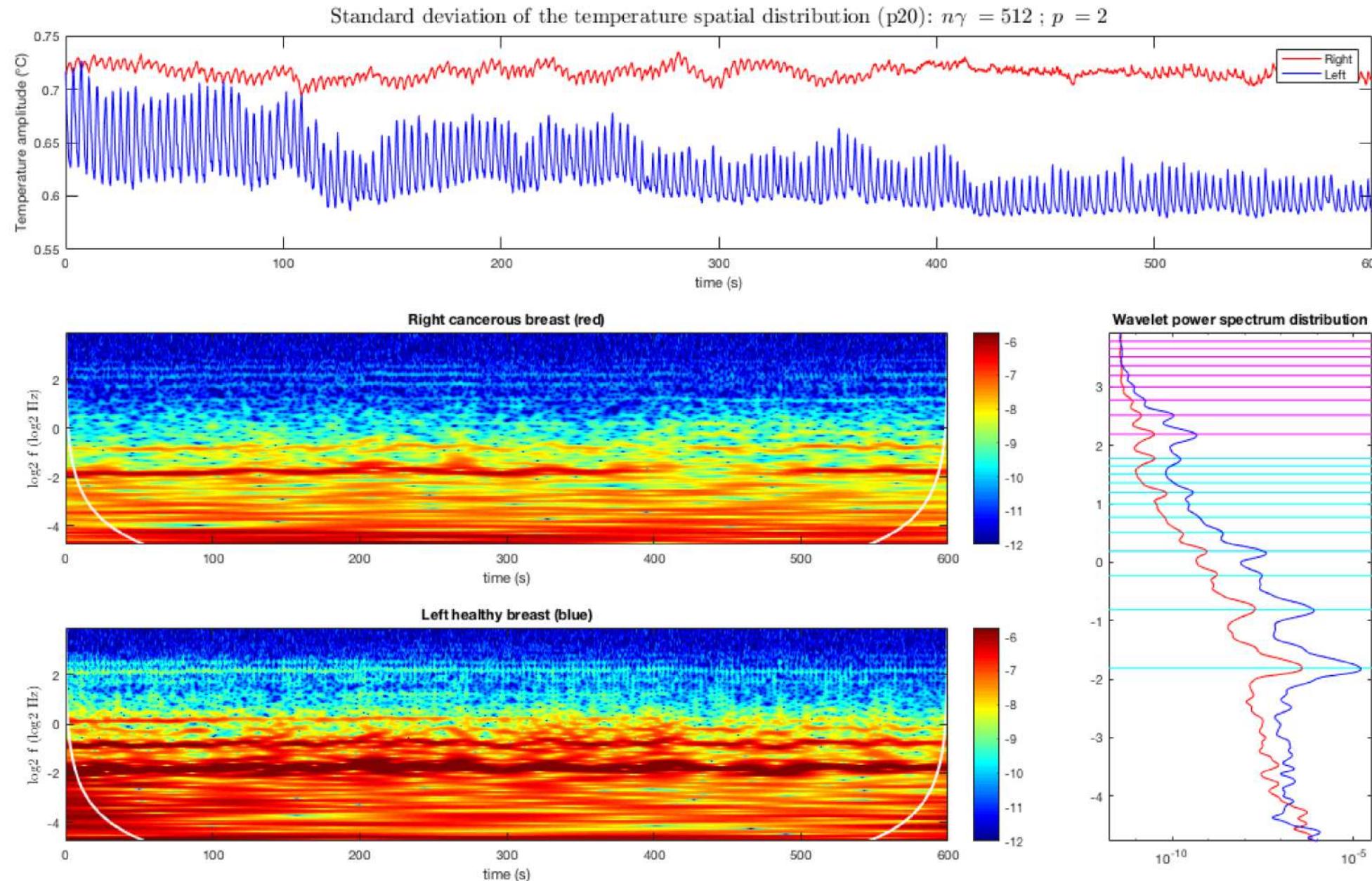


Playing on the wavelet function parameters to reveal both respiratory and cardiac rhythms

Mean of the temperature spatial distribution (p20 left):  $Q = 32$ ,  $p = \frac{1}{2}$



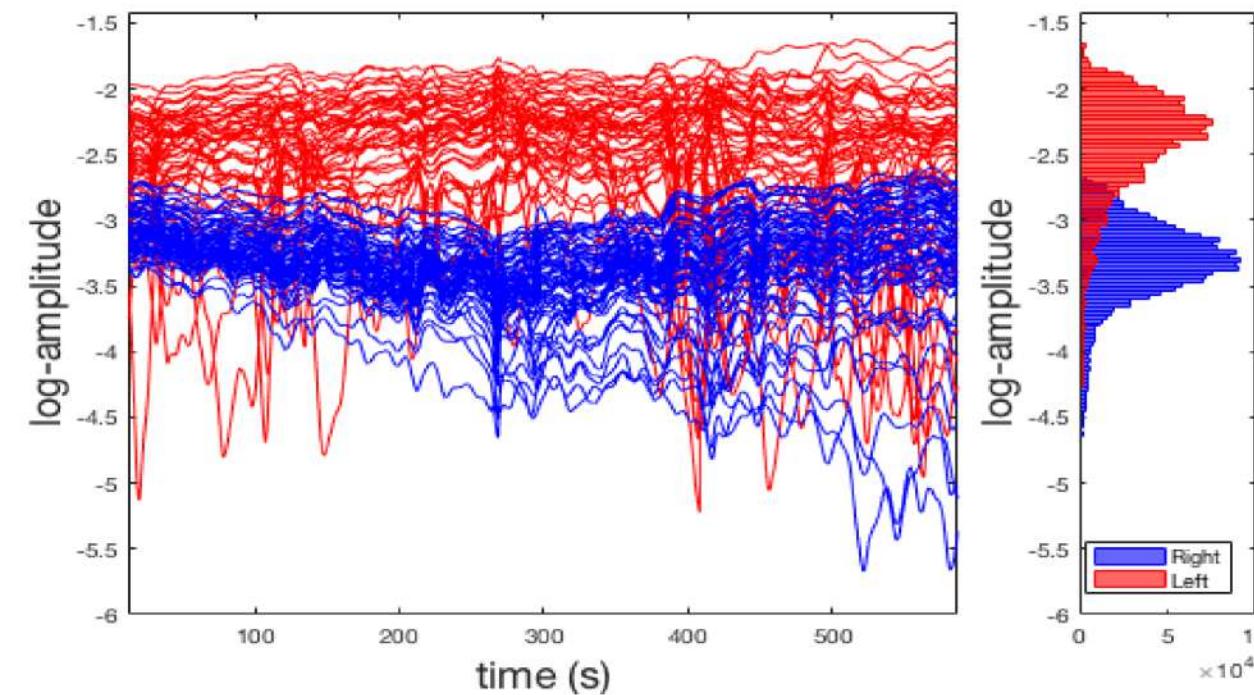
# Comparison of right (cancerous) and left (healthy) breast global temperature signals



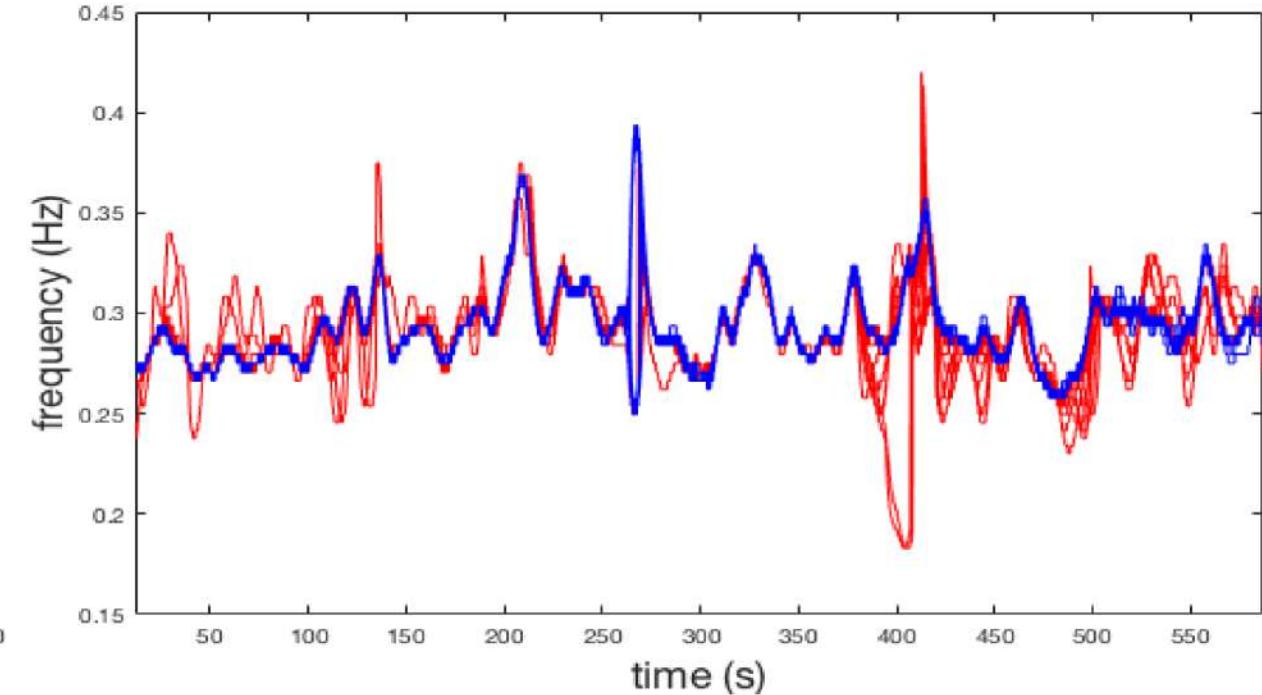
# Comparison of right (cancerous) and left (healthy) breast global temperature signals

Focusing on the respiratory rhythm fundamental on the same patient (red: cancer breast, blue healthy)

Wavelet transform amplitude modulus



Temporal evolution of the instantaneous frequency

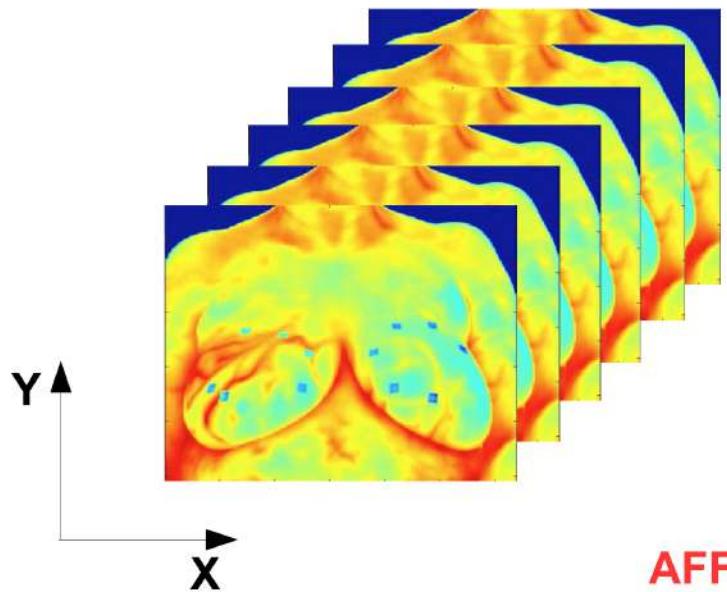


Skewed distributions  
(long tails)

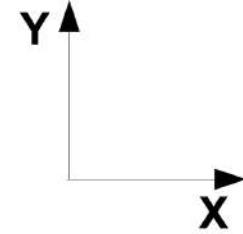
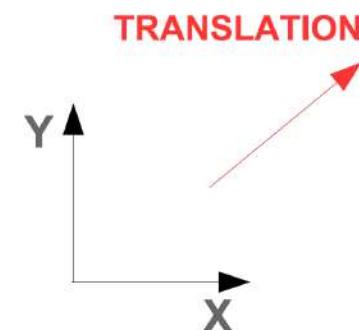
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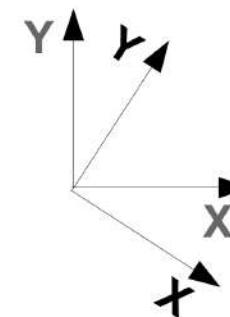
Translation and Affine algorithm to extract these displacements



**AFFINE TRANSFORMATION  
 $R_2 * D * R_1$**

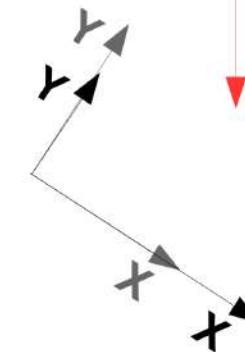
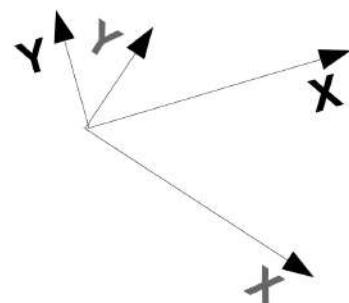


**ROTATION I:  $R_1$**



**DILATION-CONTRACTION:  $D$**

**ROTATION II:  $R_2$**



## PLAN OF THE PRESENTATION

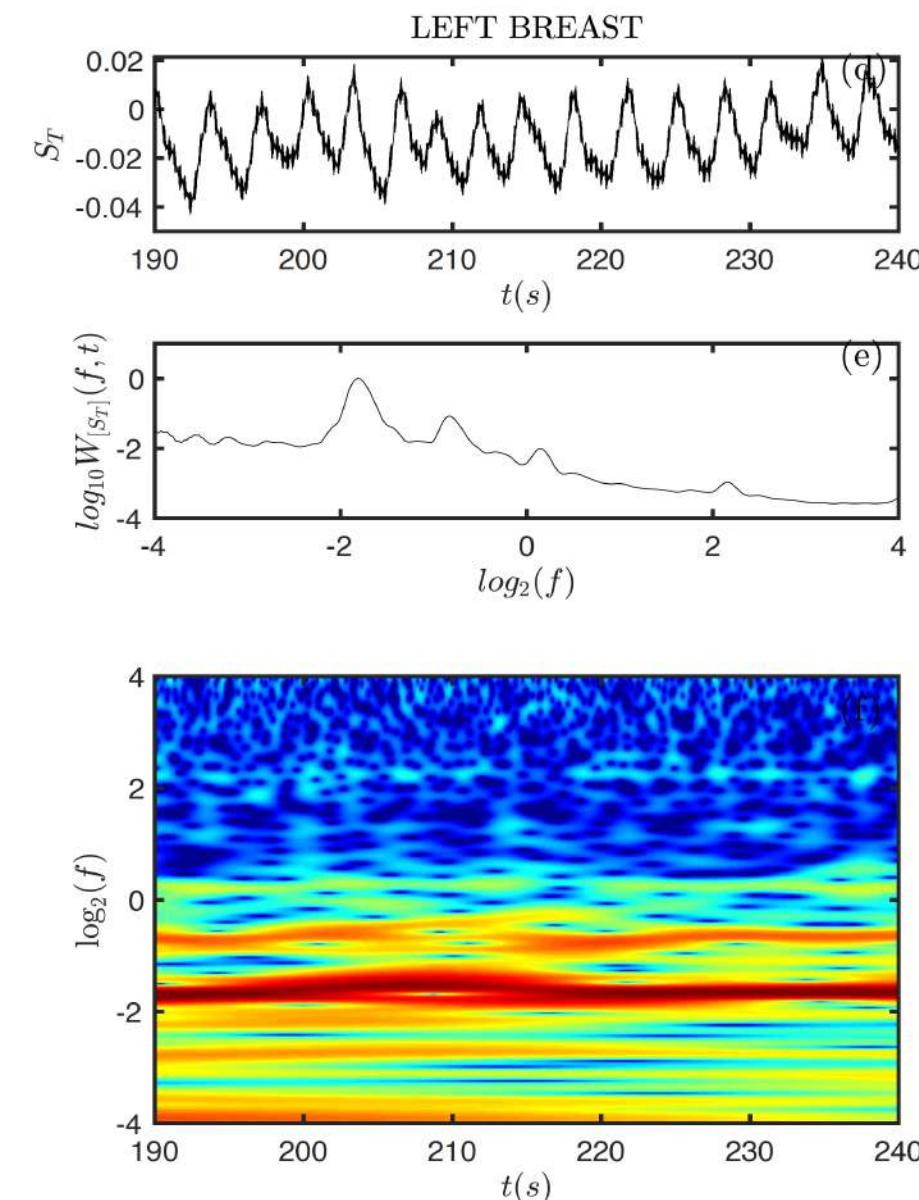
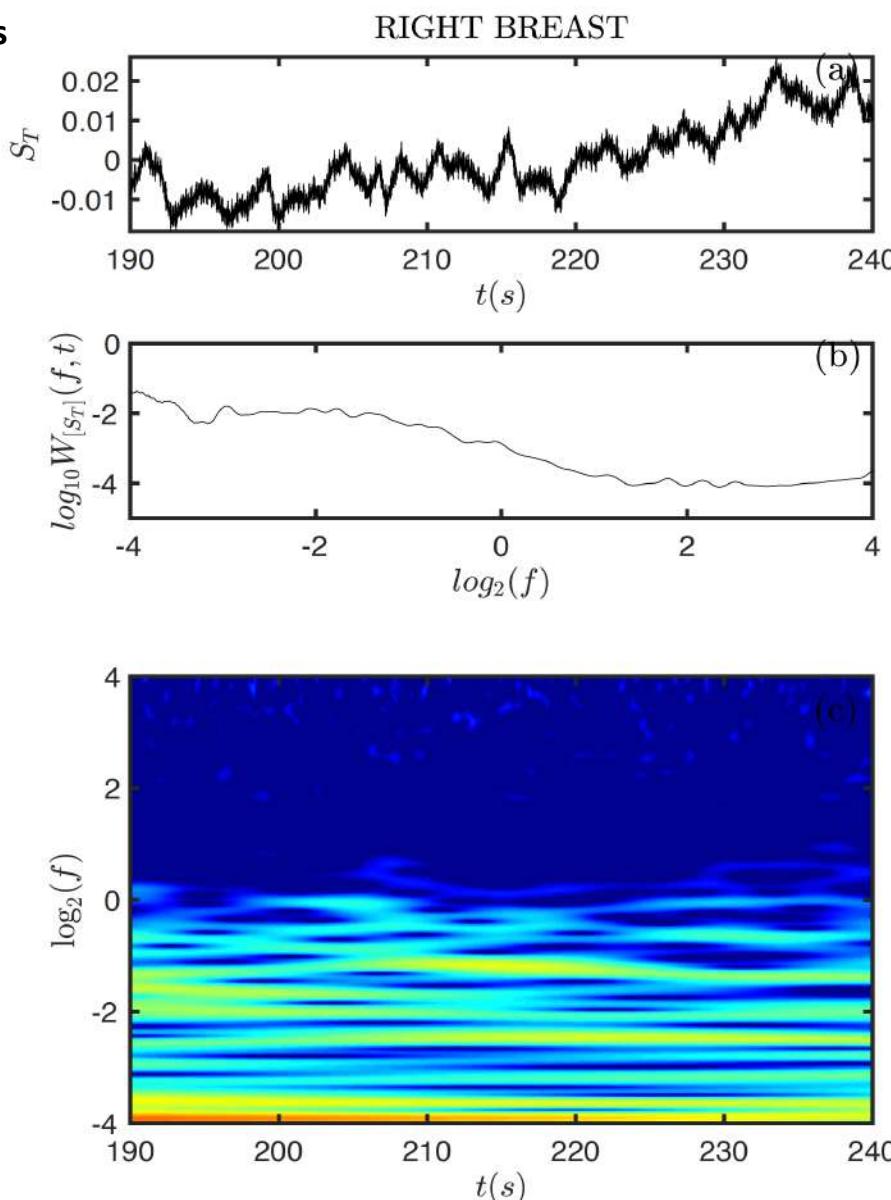
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# Comparison of time-frequency decomposition of uncorrected and corrected signals

Uncorrected signals

N=256

p=1

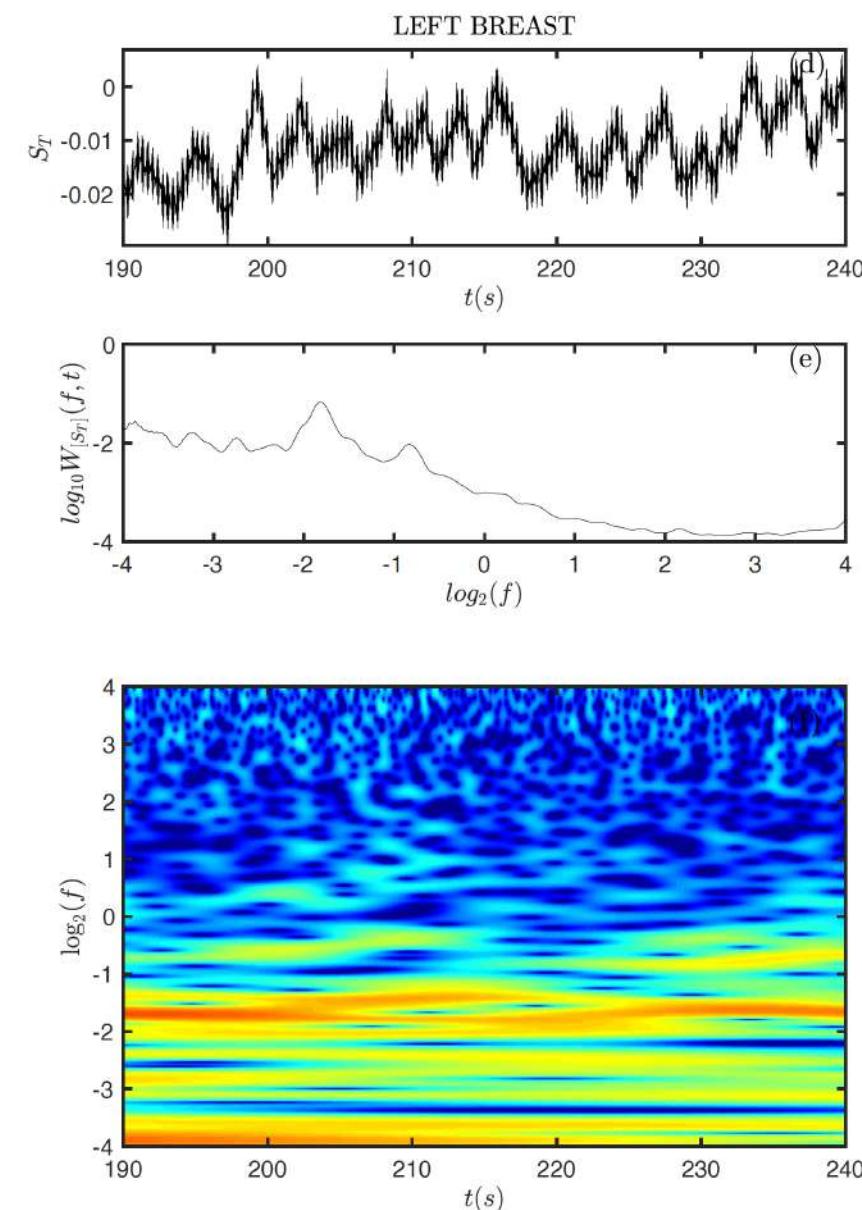
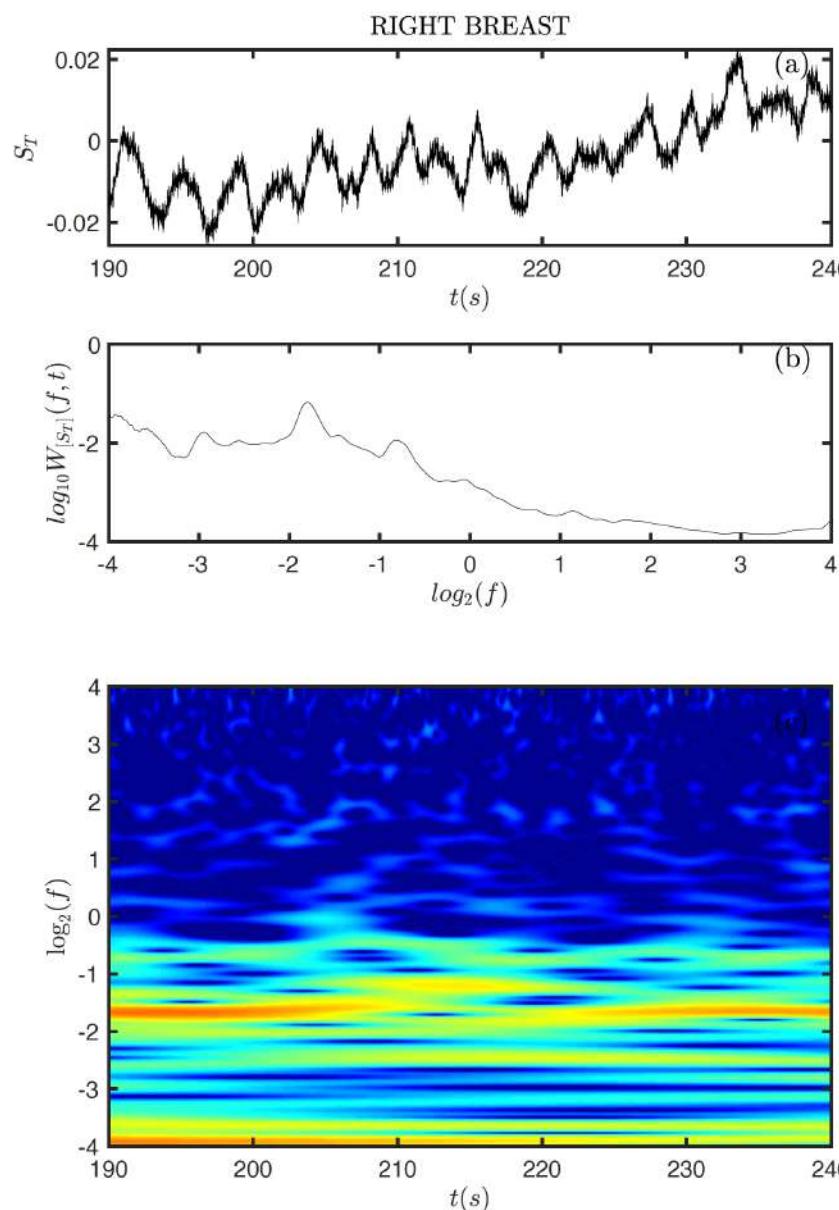


# Comparison of time-frequency decomposition of uncorrected and corrected signals

Corrected signals

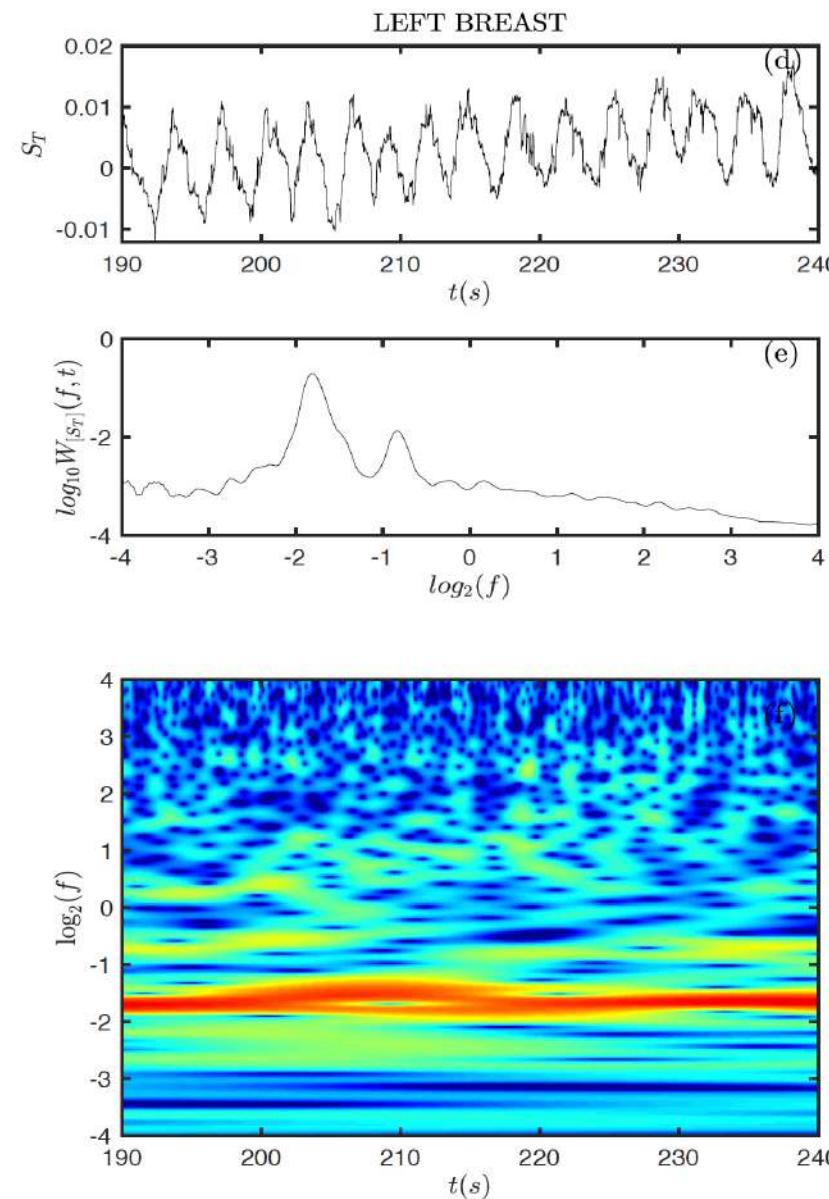
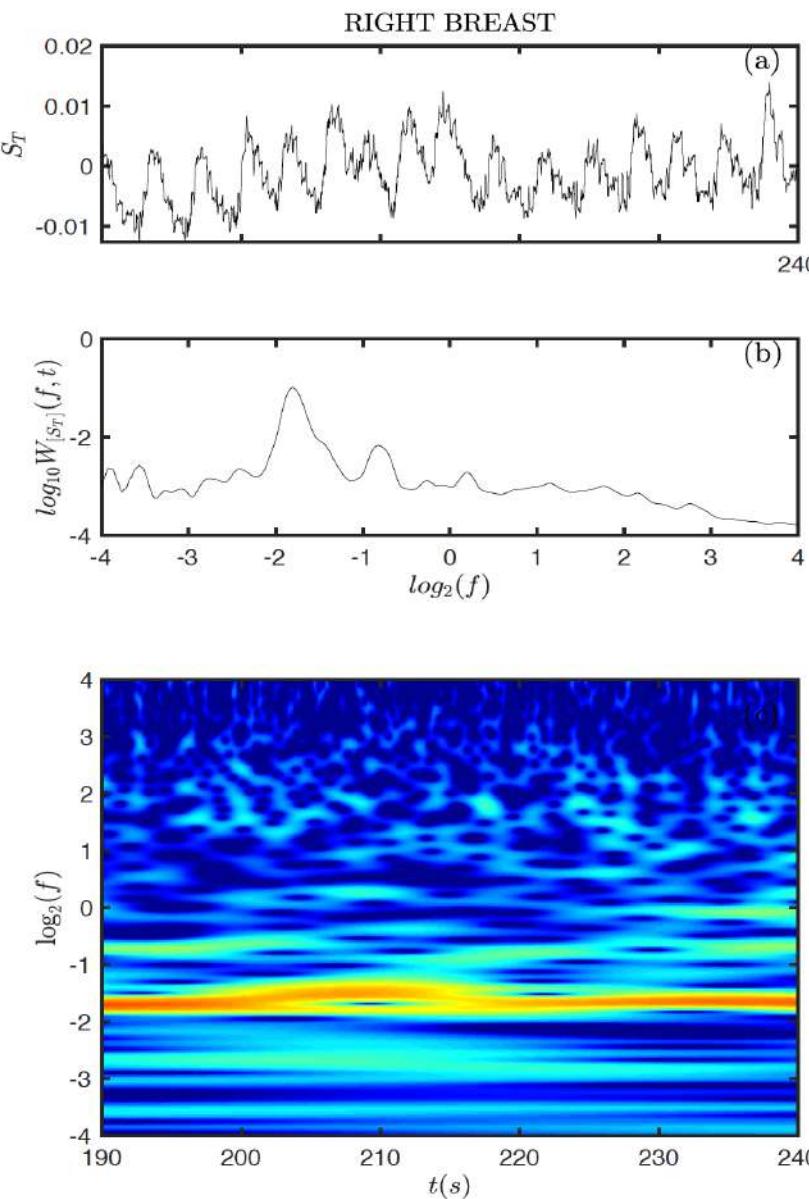
N=256

p=1



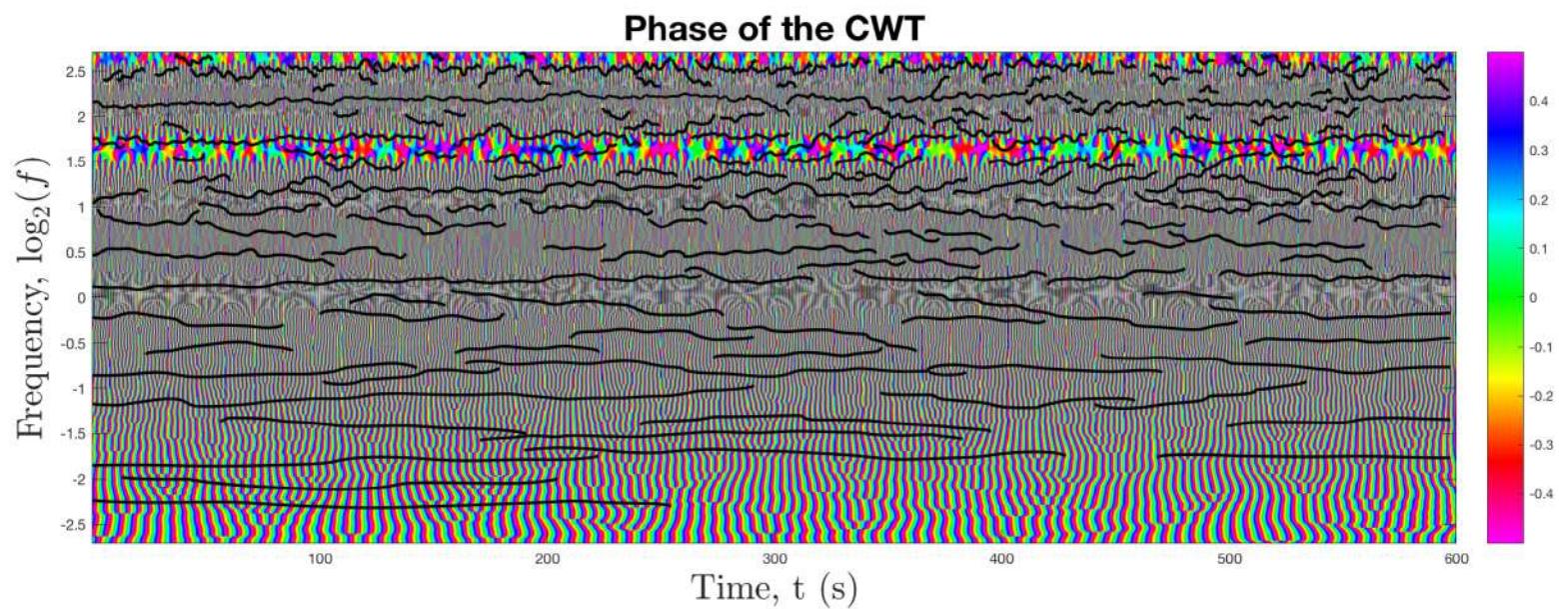
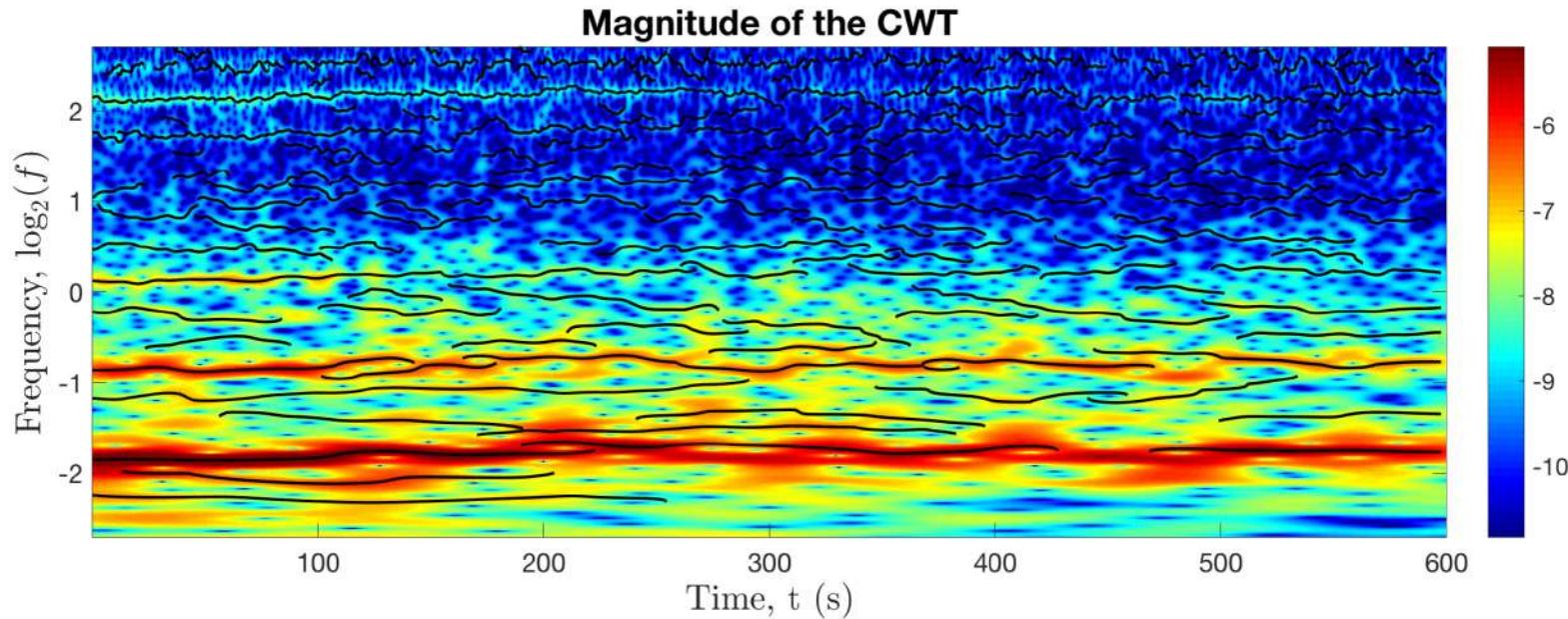
# Comparison of time-frequency decomposition of uncorrected and corrected signals

**Transformation**  
**Affine matrix**  
**determinant**  
**N=256**  
**p=1**

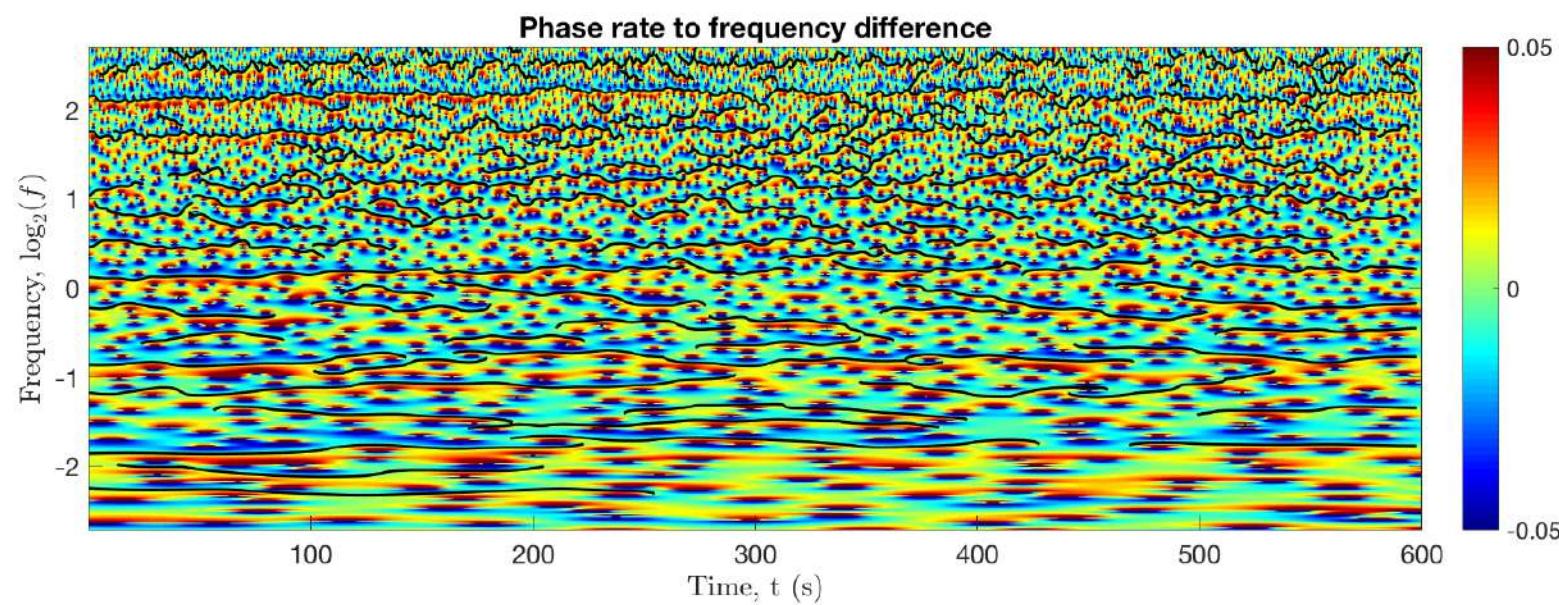
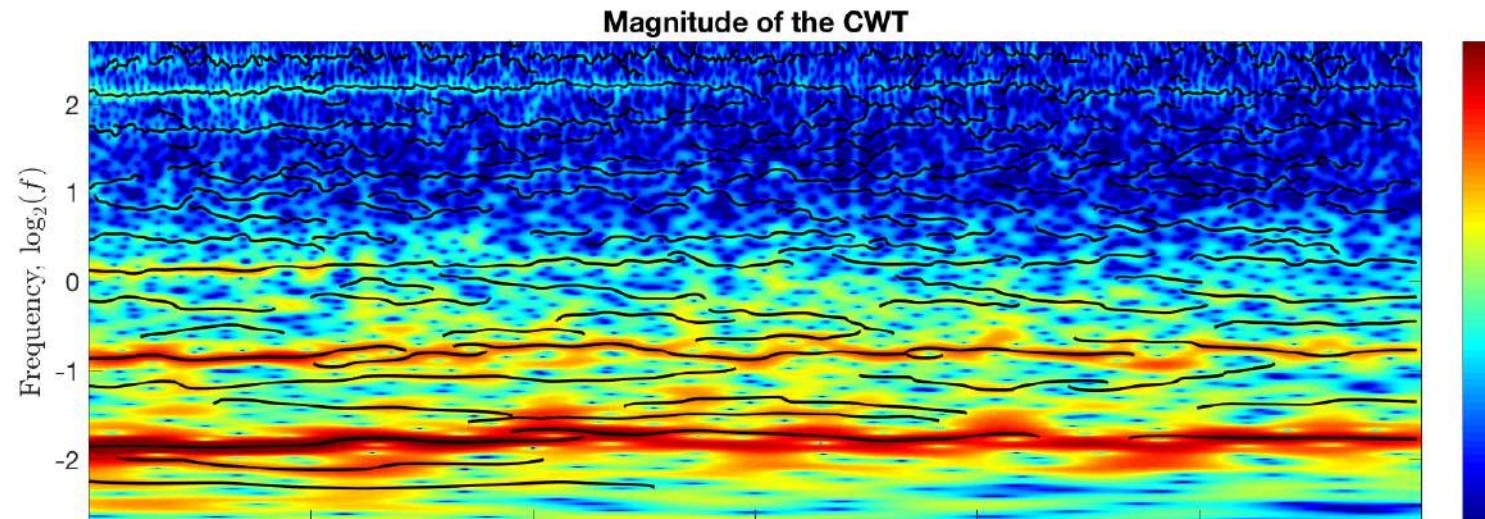


# Detection of the ridges of the CWT (from the magnitude or modulus of the CWT)

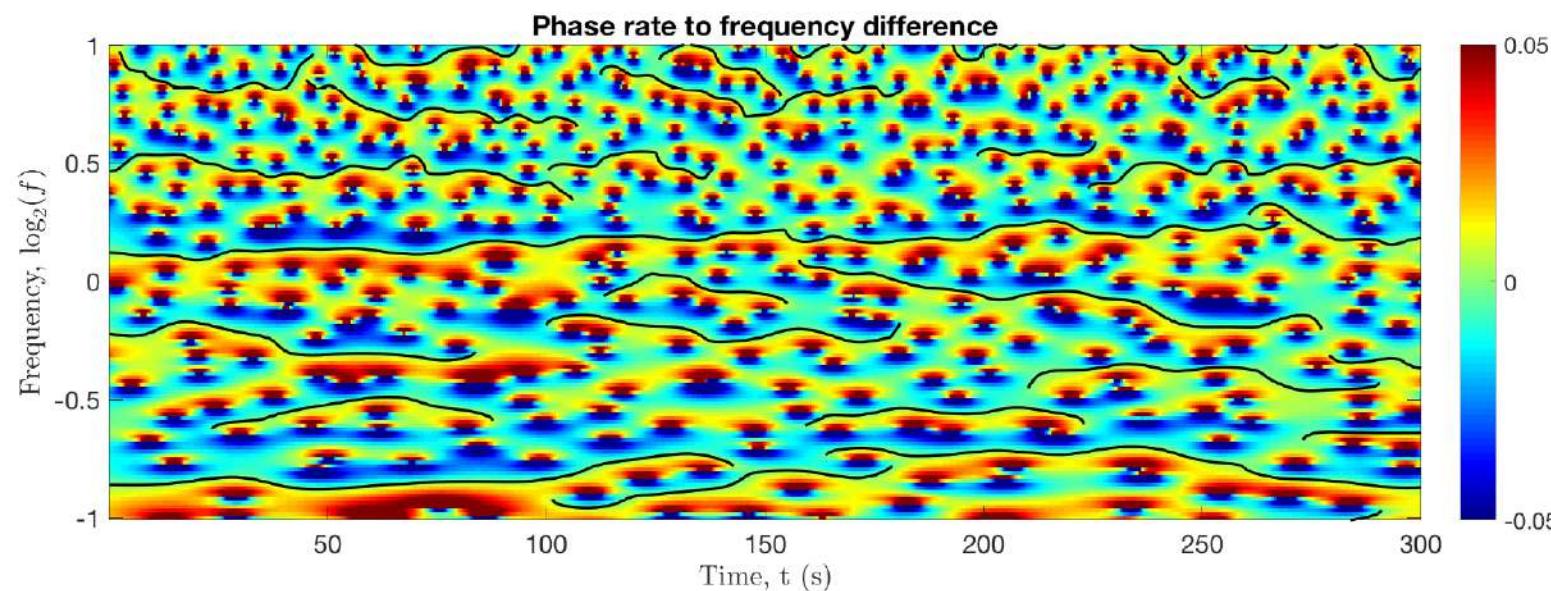
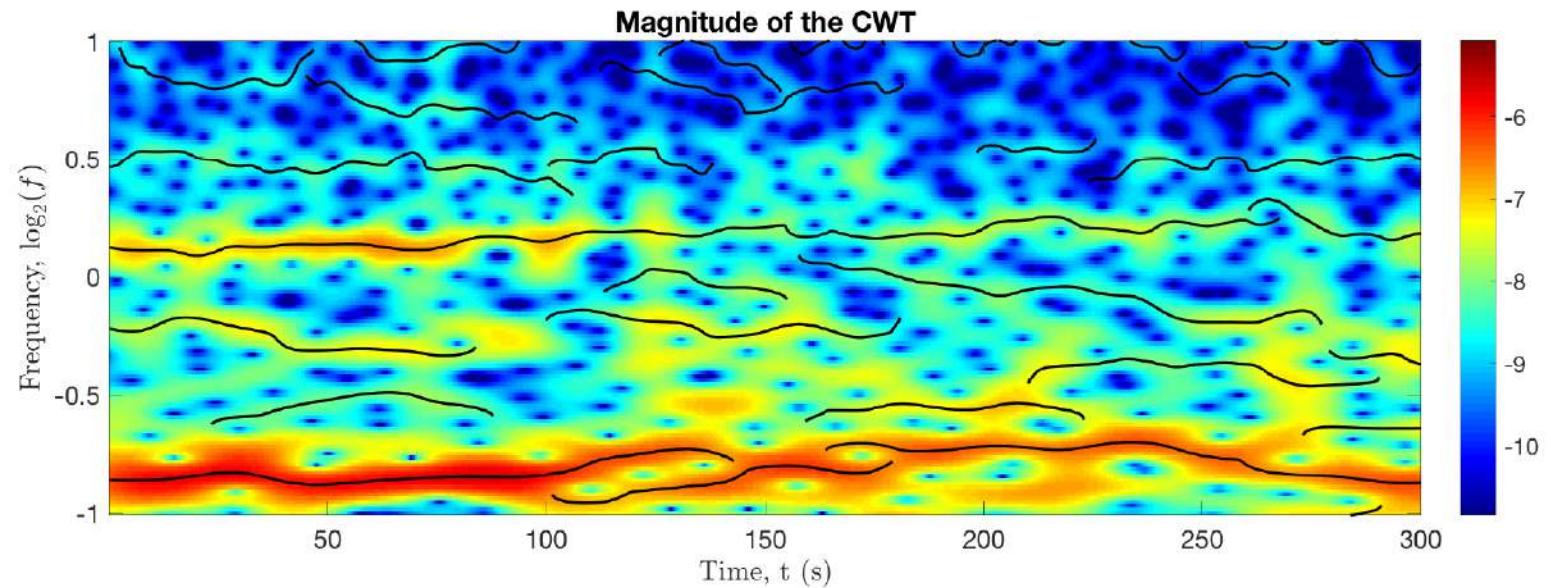
Q=32



# Detection of the ridges of the CWT (comparing modulus and phase difference methods)



# Detection of the ridges of the CWT (comparing modulus and phase difference methods)



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## Disentangling respiratory from cardiogenic rhythms

Recognition of the presence of two (or more rhythms) inside the signal: multiplicative cross-correlation of the modulus of the CWT in the frequency variable  $f$  (the integral is performed in  $\log(f)$  scales)

Here we take  $s_1 = s_2$ , the log-frequency variable for  $s_2$  is shifted by  $\log(q)$

$$R_\psi[s_1, s_2](q, t) = C_{\psi, \psi}^{-1} \int_0^\infty |W_\psi[s_1](f, t) W_\psi[s_2](qf, t)| df/f ,$$

where  $C_{\psi, \psi} = \int_0^\infty |\tilde{\psi}(f)|^2 df/f$ .

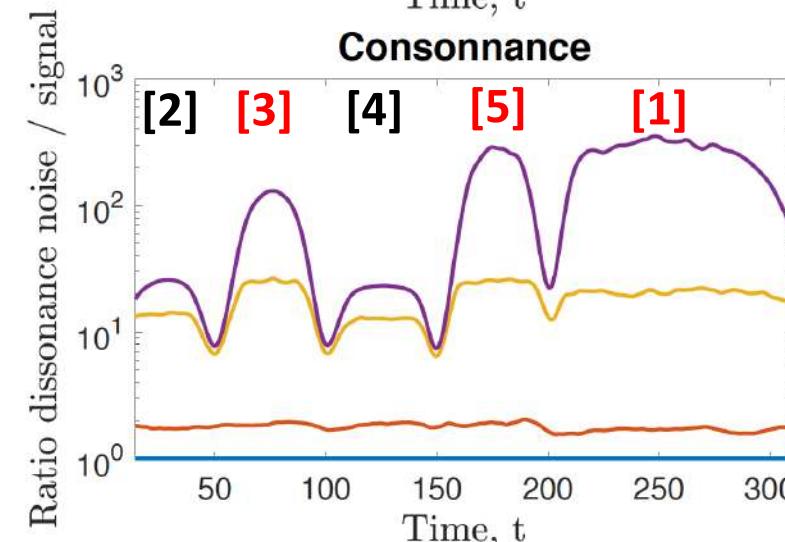
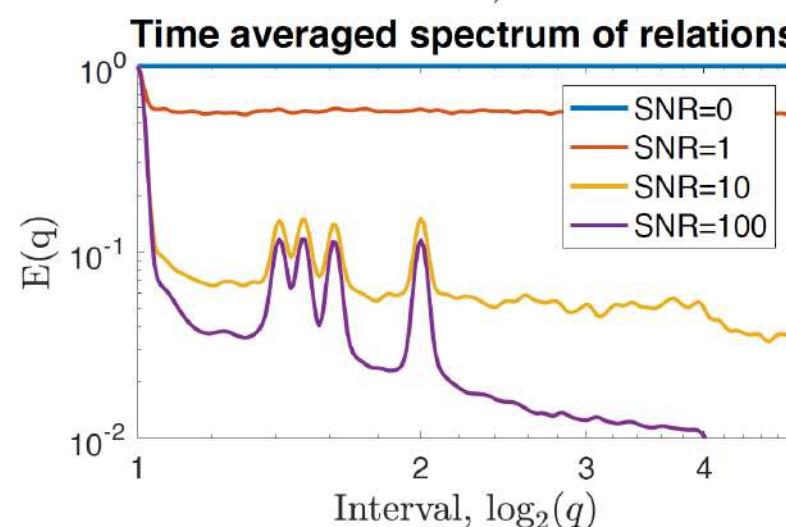
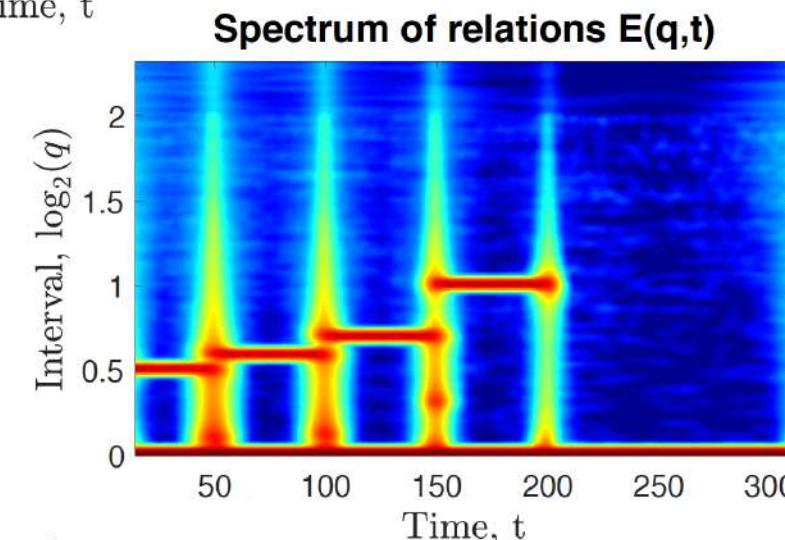
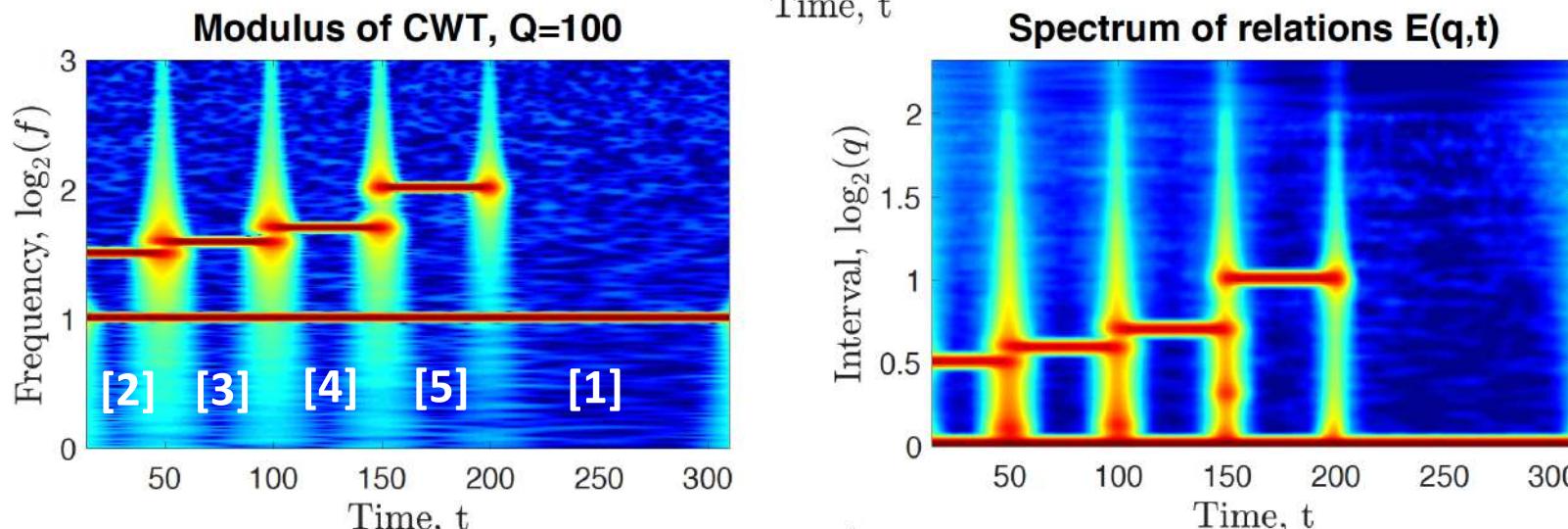
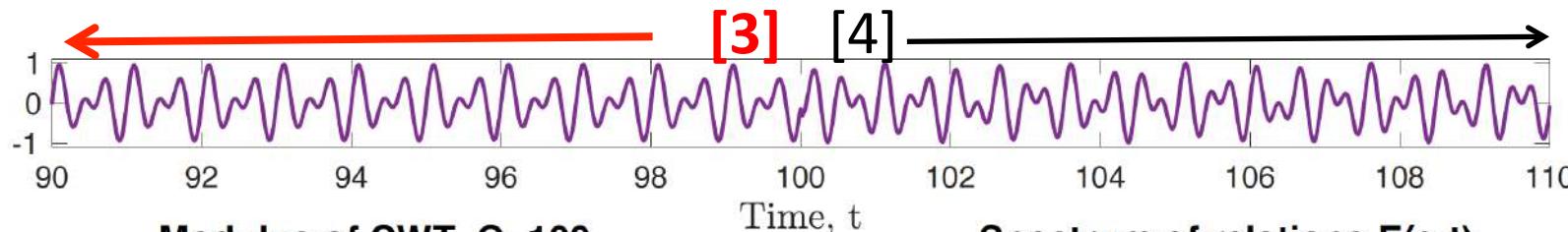
$E(q, t) = R_\psi[s_1, s_2](q, t)$  is the spectrum of relations of the two signals  $s_1$  and  $s_2$

Identification of irreducible fractions of the frequency ratios occurring in the spectrum of relations of the signal with itself -> « **consonance of the rhythms** »

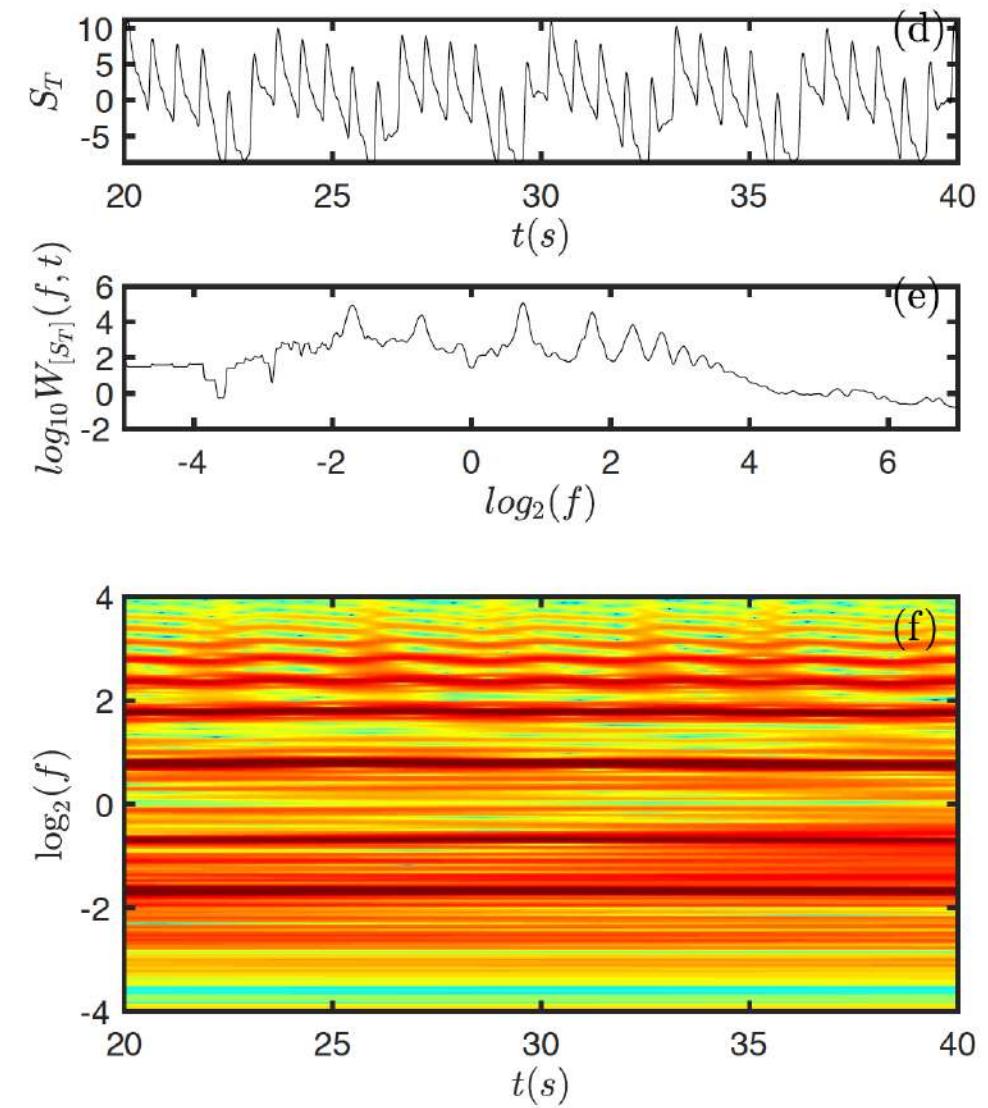
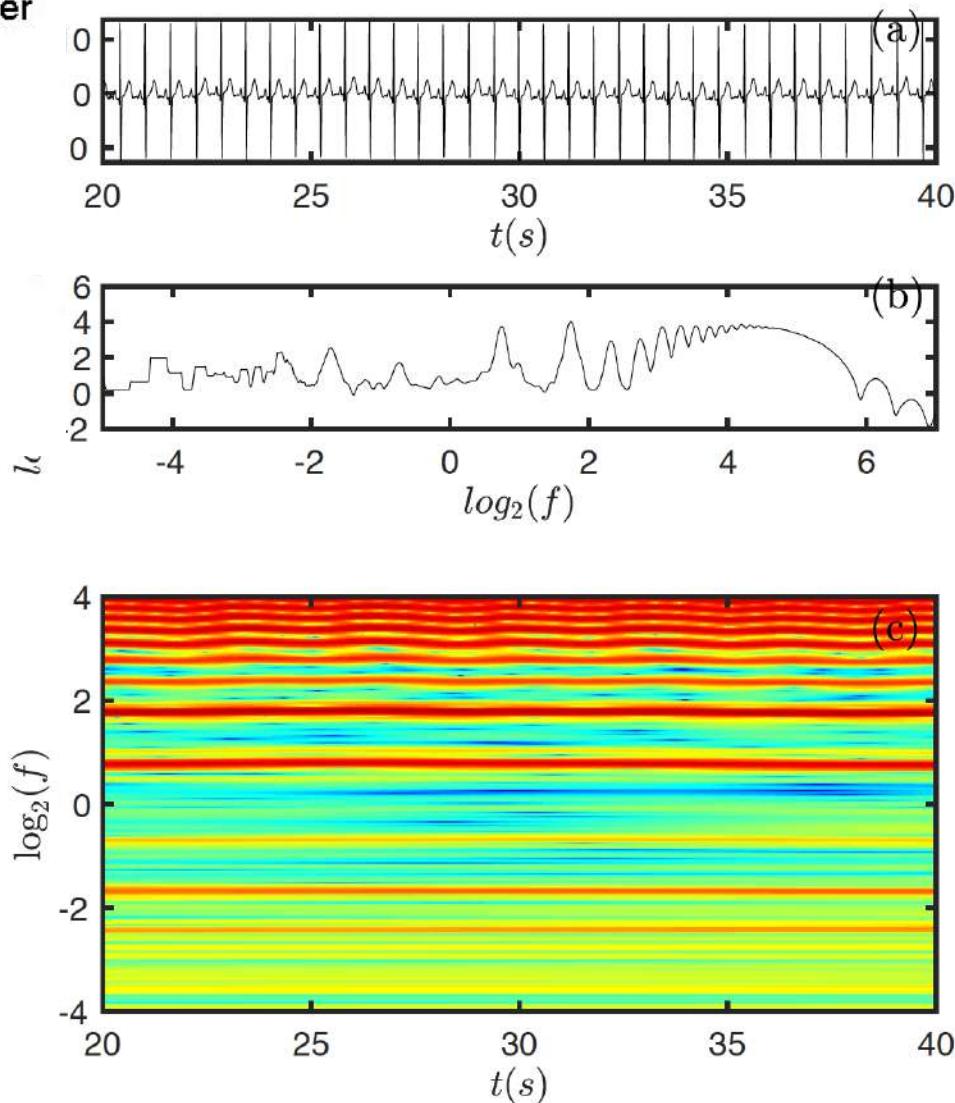
# Searching for the “consonance” of a synthetic signal

## Rhythm ratios

- [1] **1**
- [2]  $\sqrt{2}$
- [3]  **$3/2$**
- [4]  $(\sqrt{5} + 1)/2$  (golden)
- [5] **2**



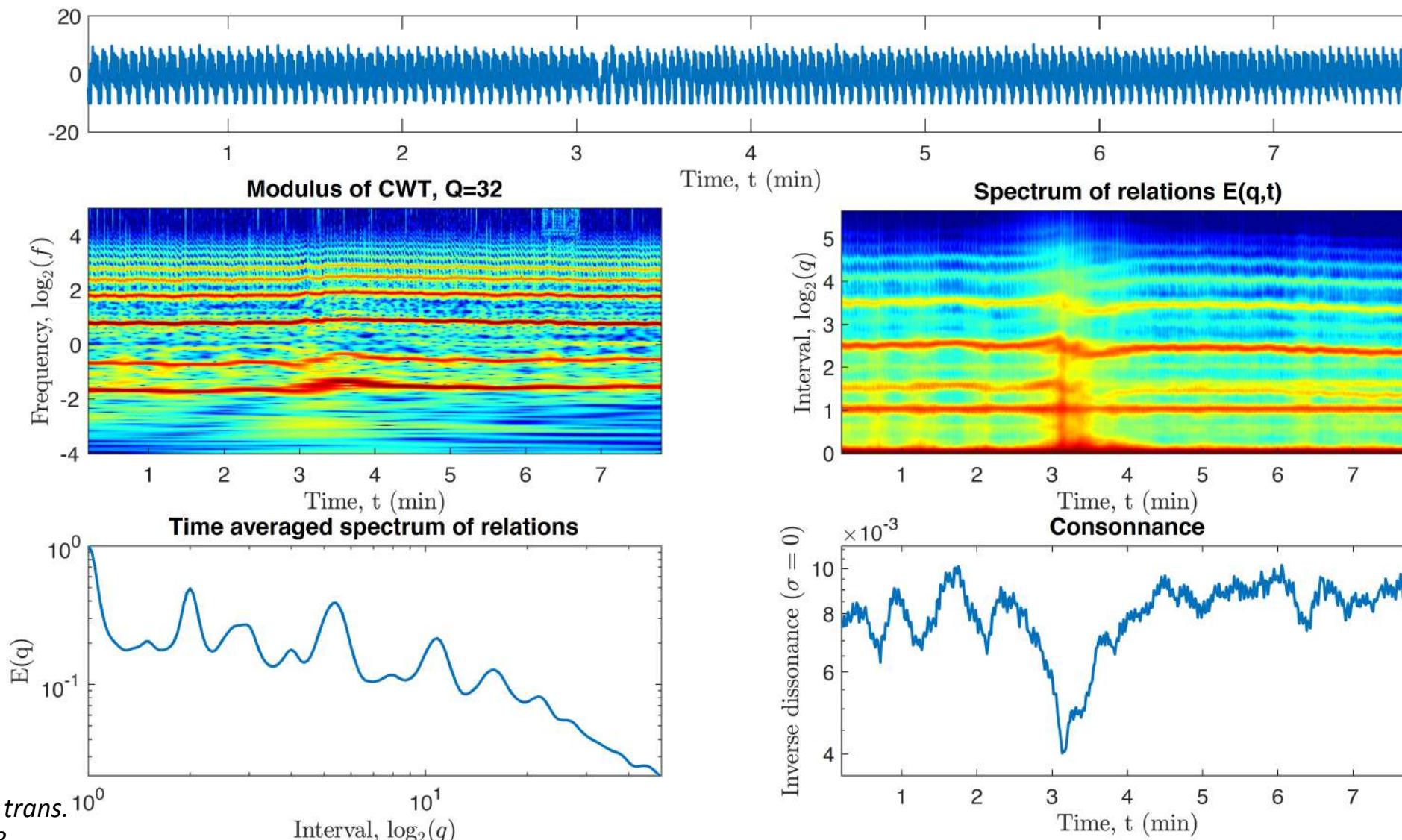
# CWT analysis of photoplethysmogram signals



W. Karlen et al., IEEE trans.  
on biomed Eng. 2013,

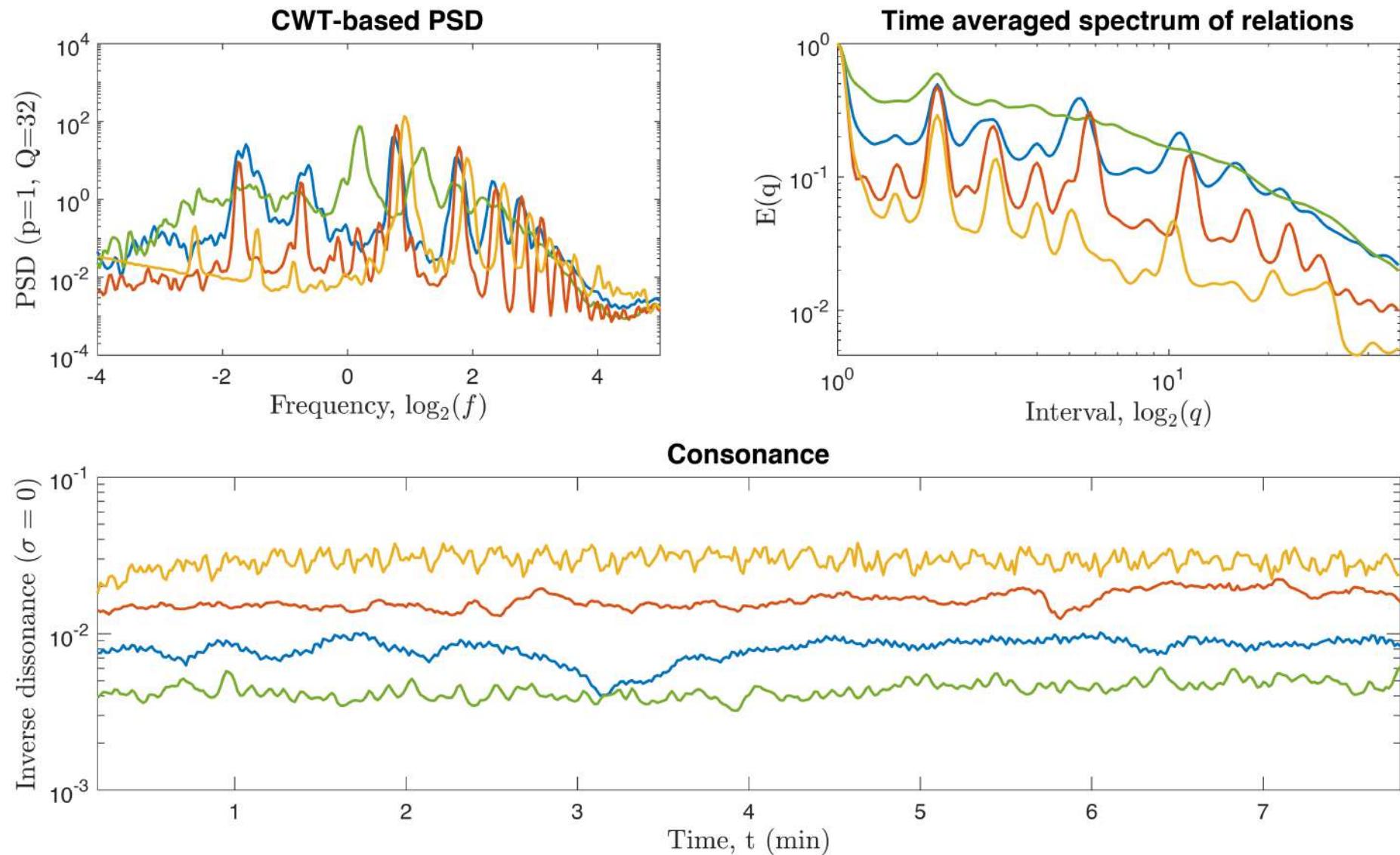
Signals downloaded from  
<http://www.capnibase.org/index.php?id=857>

# Wavelet based computation of consonance of photoplethysmogram signals



W. Karlen et al., IEEE trans. on biomed Eng. 2013,

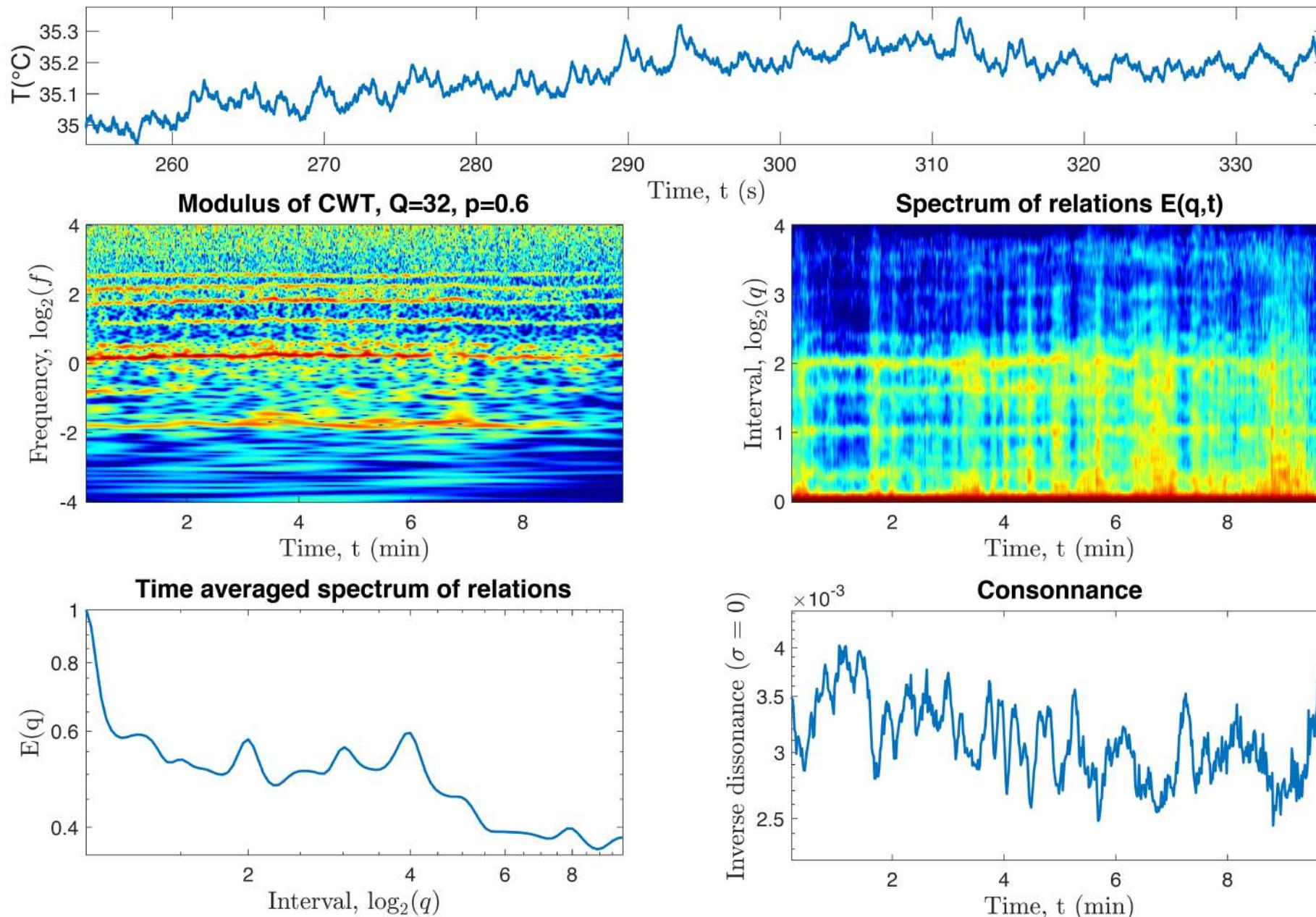
# CWT analysis of photoplethysmogram signals



W. Karlen et al., IEEE trans.  
on biomed Eng. 2013,

Signals downloaded from  
<http://www.capnibase.org/index.php?id=857>

# Wavelet based computation of the consonance of a thermogram signal



## CONCLUSIONS

**Time-frequency decomposition allows a complete characterization of the intertwining of rhythms in physiology**

**The introduction of consonance (or disonance) of rhythm ratios and its temporal change (or variability)  
as a marker of the dynamical adjustement of the body**

**Can this quantity be used as a ‘dynamical’ hint for assisting clinician diagnosis?**

**Statistical tests on large data sets need to be performed**

**A statistical physics formalism accounting for the spectrum of rhythm ratios is currently under progress  
(in the same line as the singularity spectrum has been elaborated for fractal signals)**