

New results from the sensor human brain project alternative

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Focus of the century: Understanding the brain

- **Human brain project:**

Aims at accomplishing the goal by re-building
the brain physiology (reminds me of Chomsky's critique
regarding understanding the nature of language!)

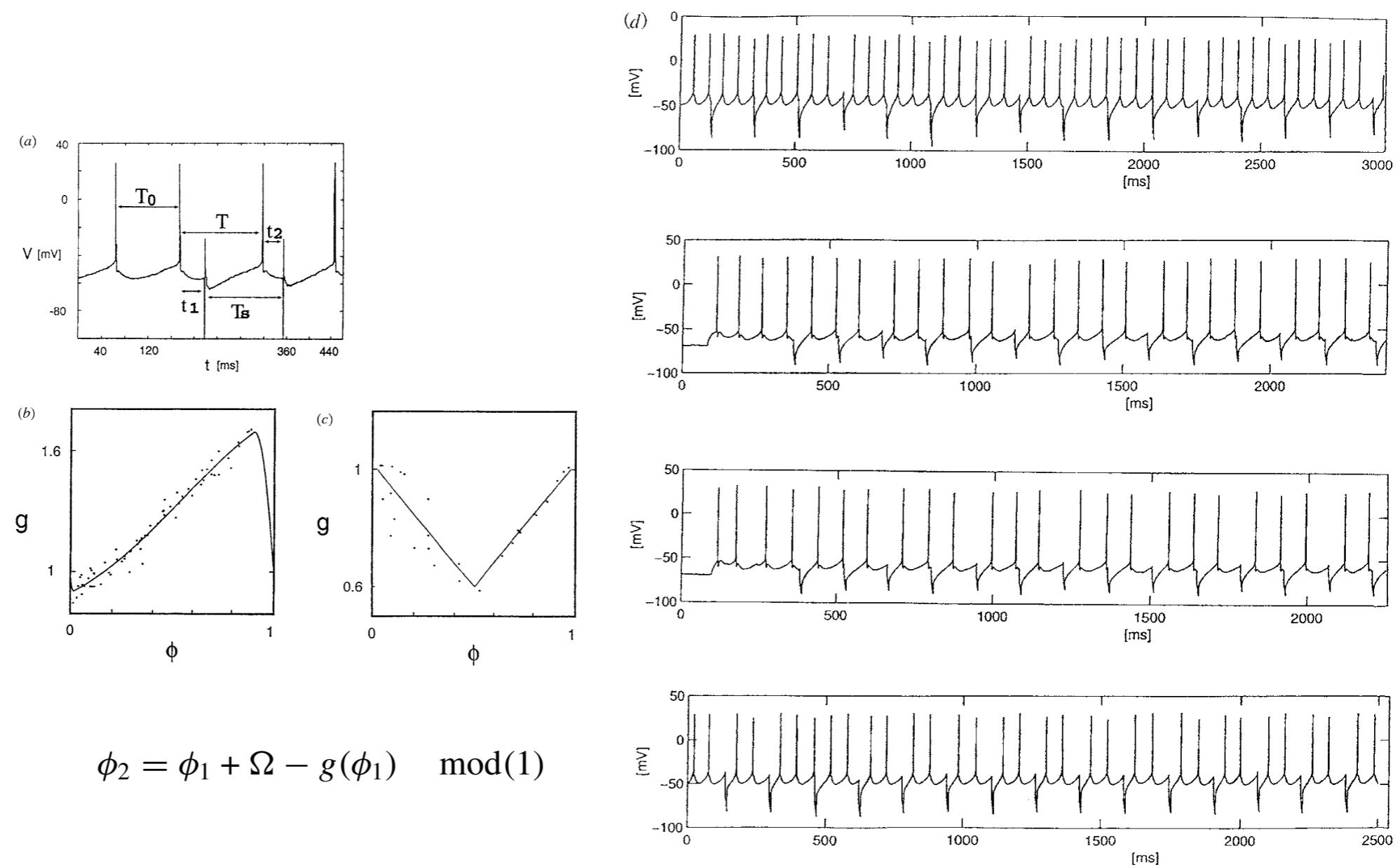
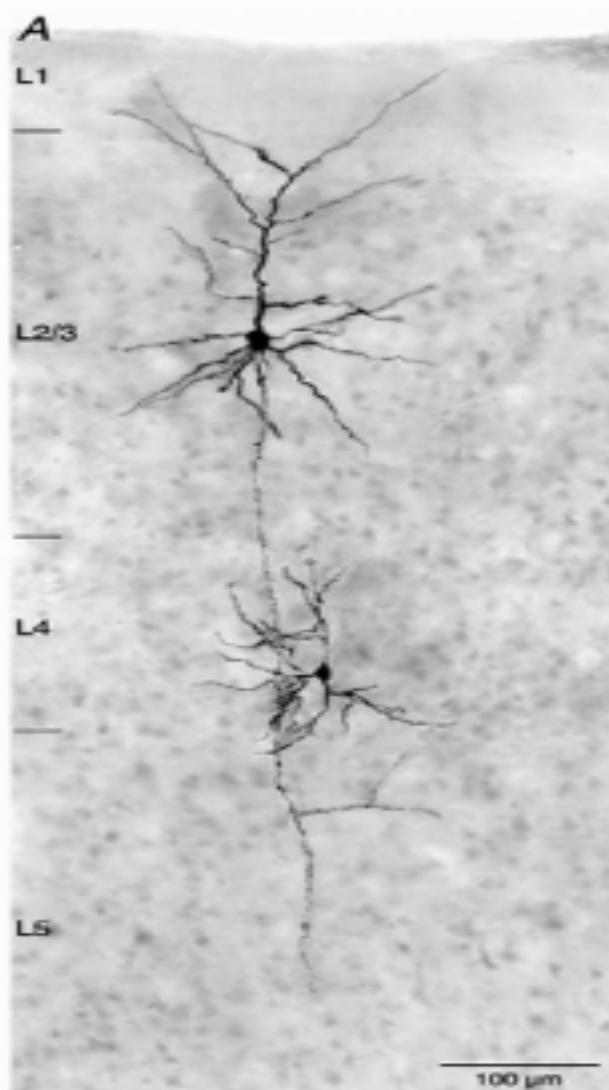
Old results that made us look for an alternative approach...

Starting 1996 @ ini UZH/ETHZ: Experiments on rat somatosensory neurons

'NEURONS ARE (JUST) OSCILLATORS' (E. Moses, Madrid 2018)

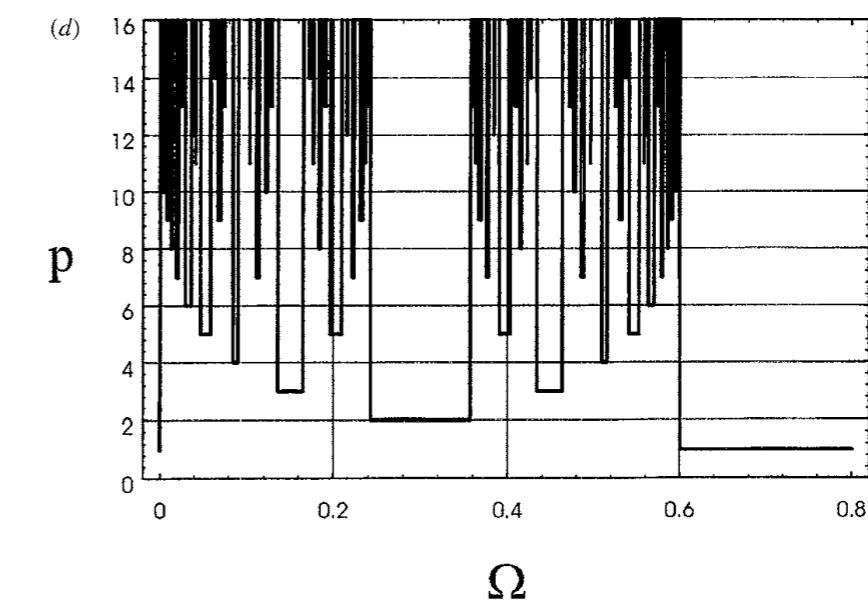
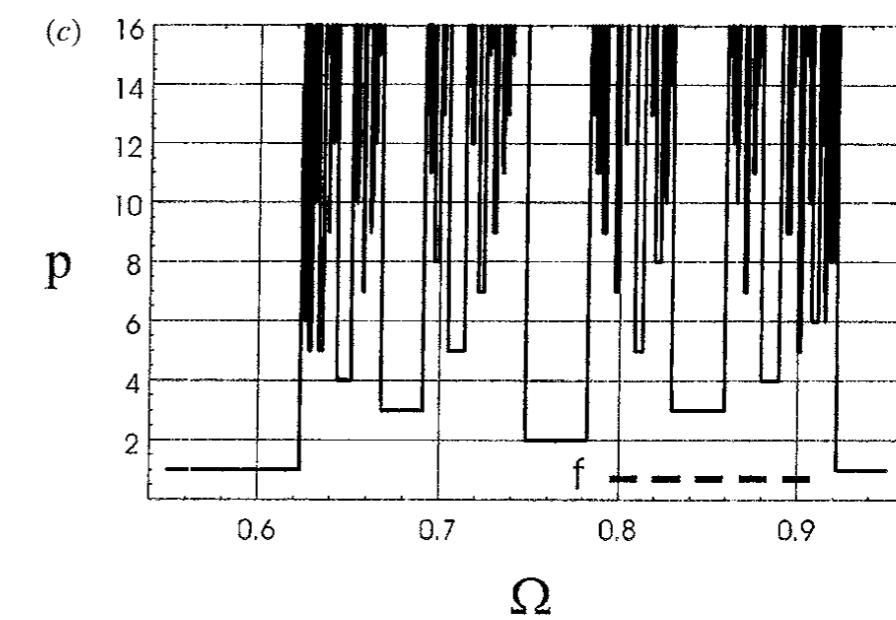
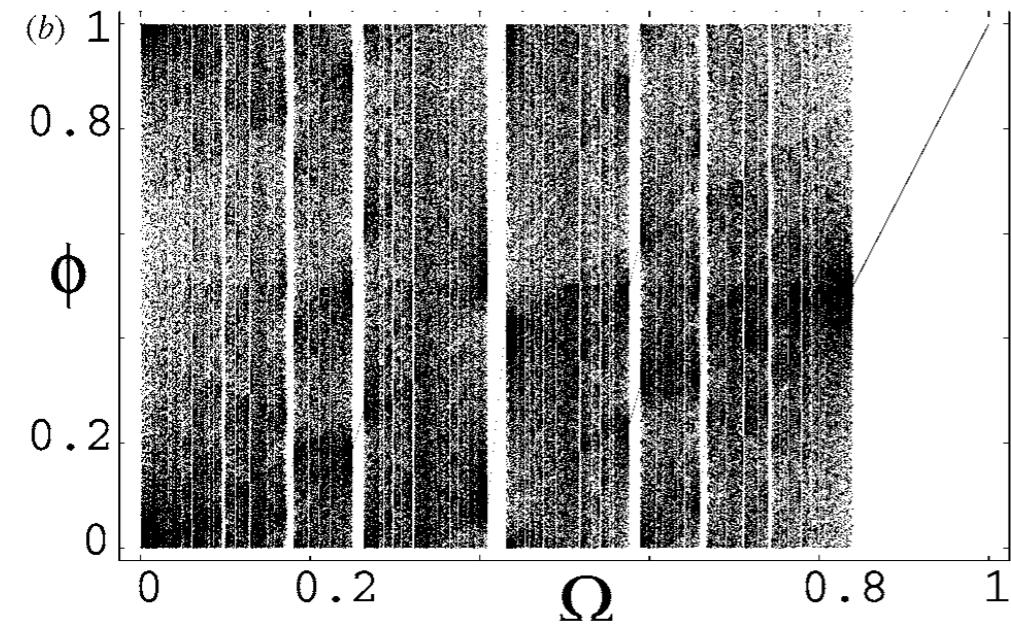
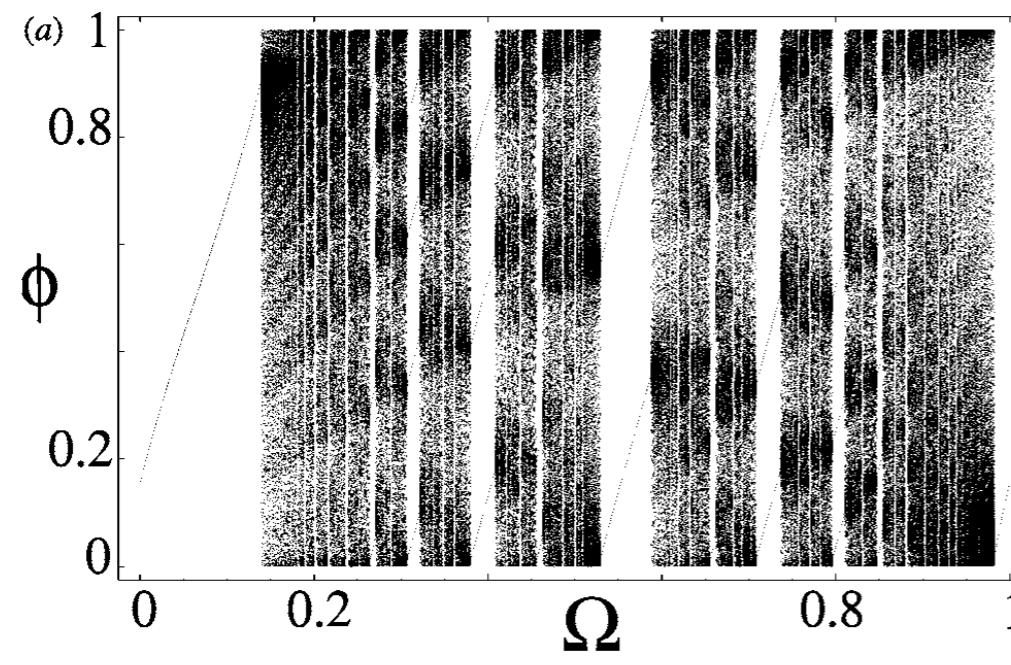


Experiments (1996/7, K. Schindler, L. Bunimovich)

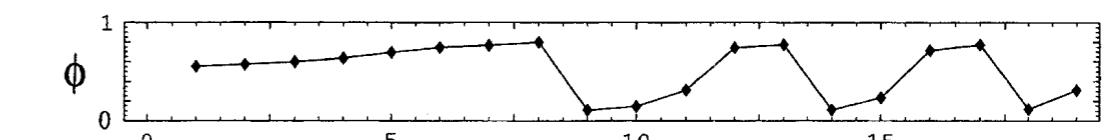
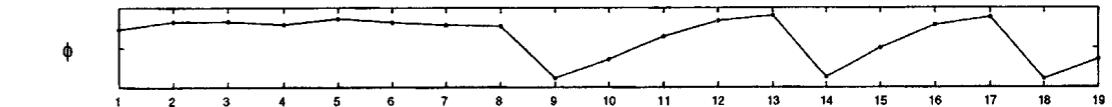
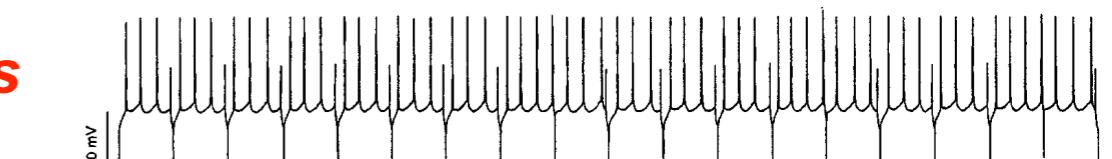
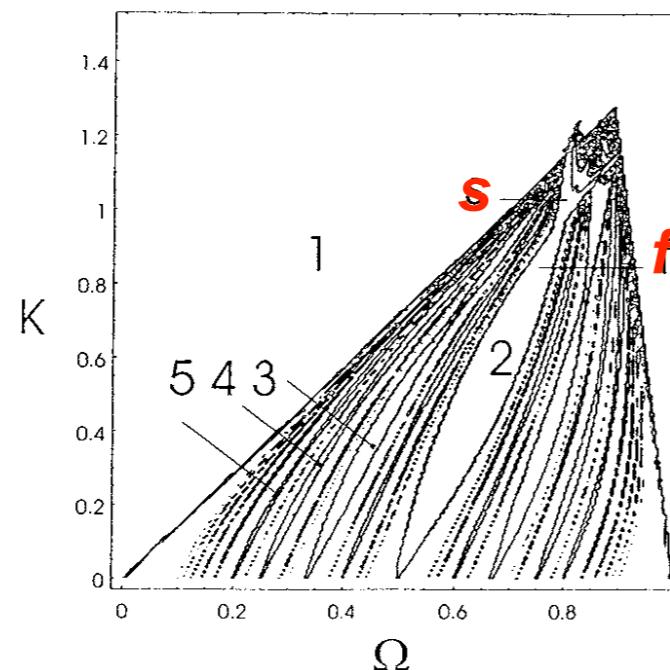
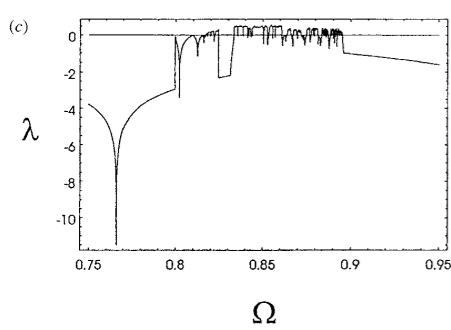
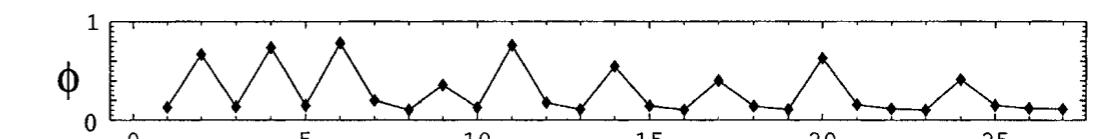
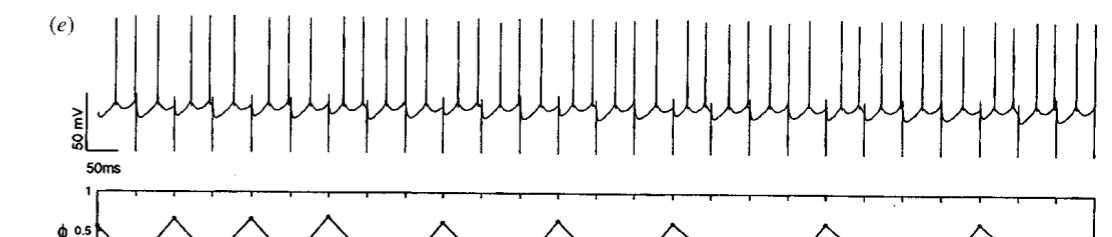
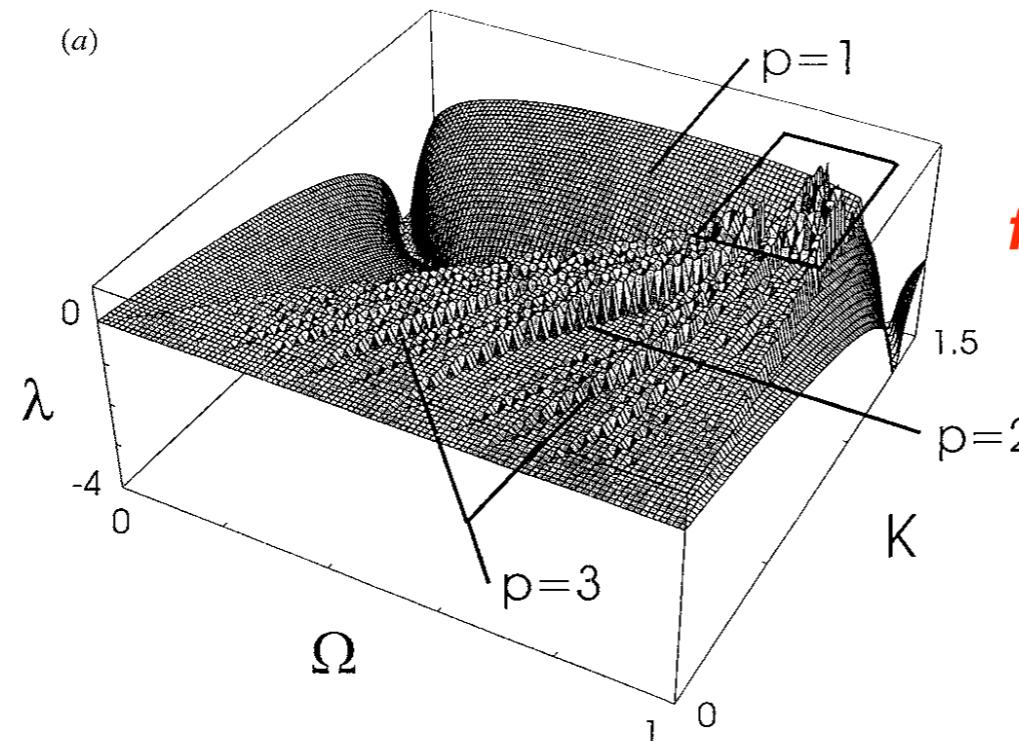




Numerical explorations:

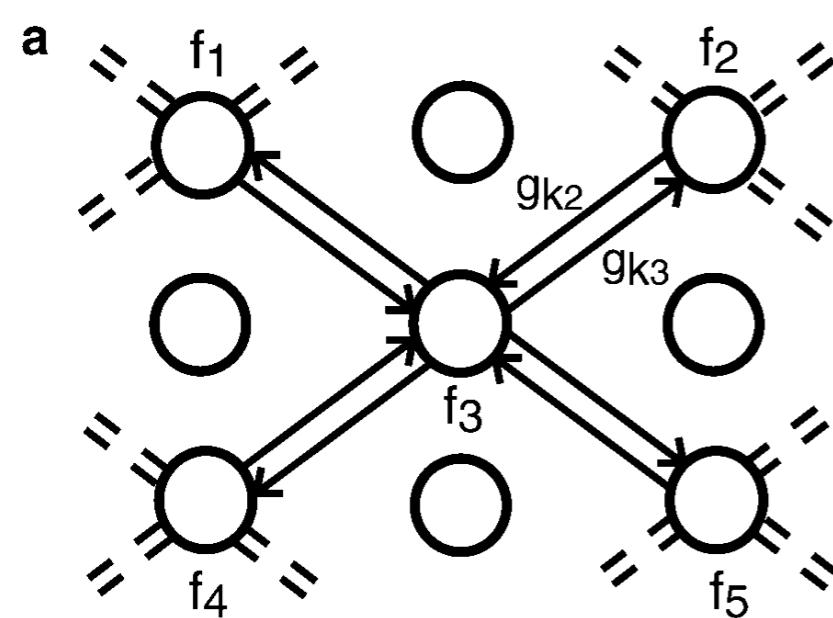


Comparison experiment-simulation:

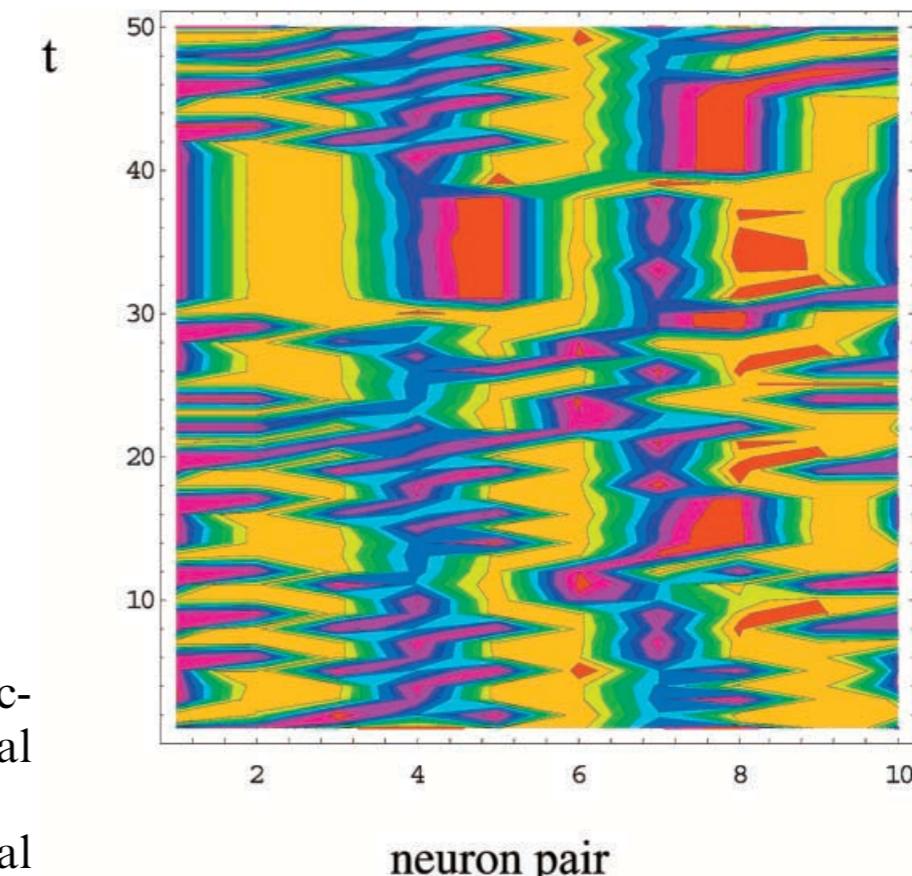


More recent generalizations:
S. Martignoli
K. Kanders

Interacting neuron pairs (1998):



$$\begin{aligned}\phi\{i,j\}(t_{n+1}) := & (1 - k_2 k\{i,j\}) f_{K\Omega}(\phi\{i,j\}(t_n)) \\ & + k_2 / nn \ k\{i,j\} \sum_{nn} \phi\{k,l\}(t_n)\end{aligned}$$



1-d chain of diffusively coupled (binary) interaction maps:

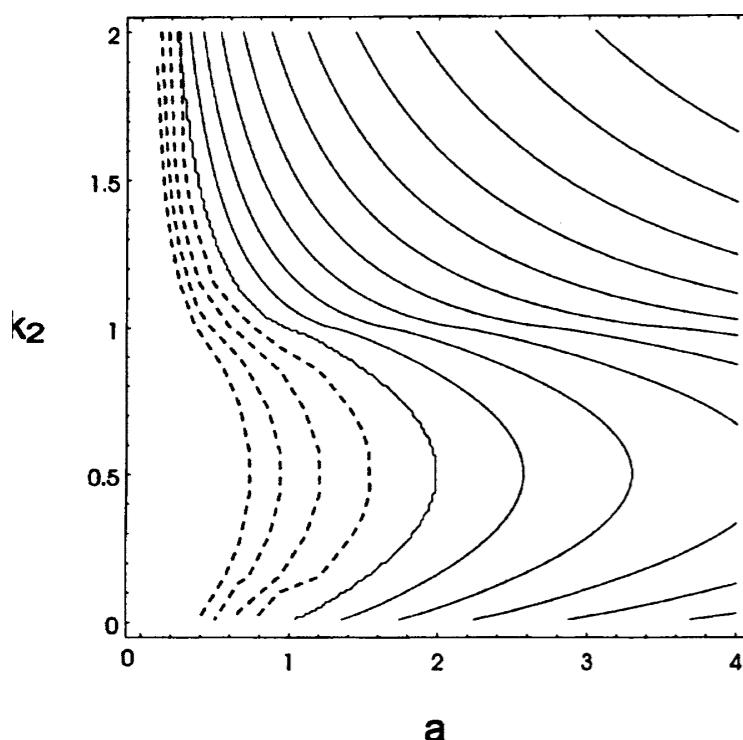
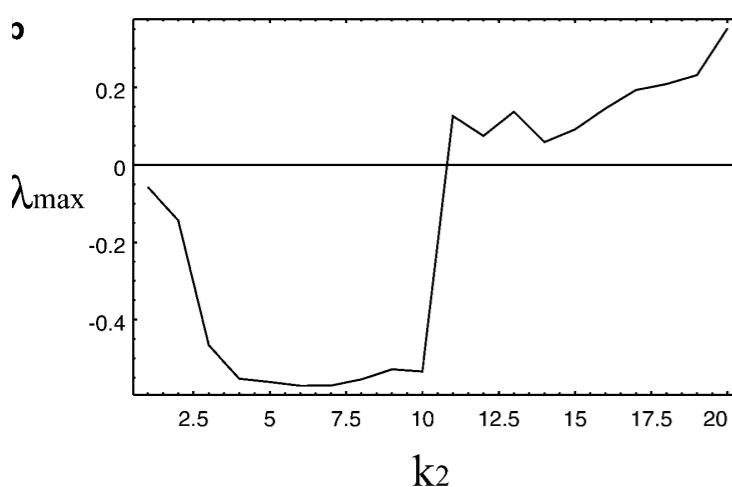
Stoop R, Schindler K, Bunimovich LA (1999) Inhibitory connections enhance pattern recurrence in networks of neocortical pyramidal cells. *Phys Lett A* 258: 115–122

Stoop R, Schindler K, Bunimovich LA (2000a) When pyramidal neurons lock, when they respond chaotically, and when they like to synchronize. *Neurosci Res* 36: 81–91

Stoop R, Schindler K, Bunimovich LA (2000b) Noise-driven neocortical interaction: complex neuron spiking uncovered by nonlinear dynamics. *Acta Biotheor* 48: 149–171

Interacting neuron pairs (1998, RS, LAB, WHS):

1-d chain of diffusively coupled
 (binary) tent-map (slope a) interaction maps:

**a**

Phase-coincidence learning $k\{i,j\}(t_{n+1}) := k\{i,j\}(t_n)(\text{Tanh}[r] + 1)/2$
(binary) tent-map (slope a) interaction maps
 (r=sum of absolute inverse phase differences)

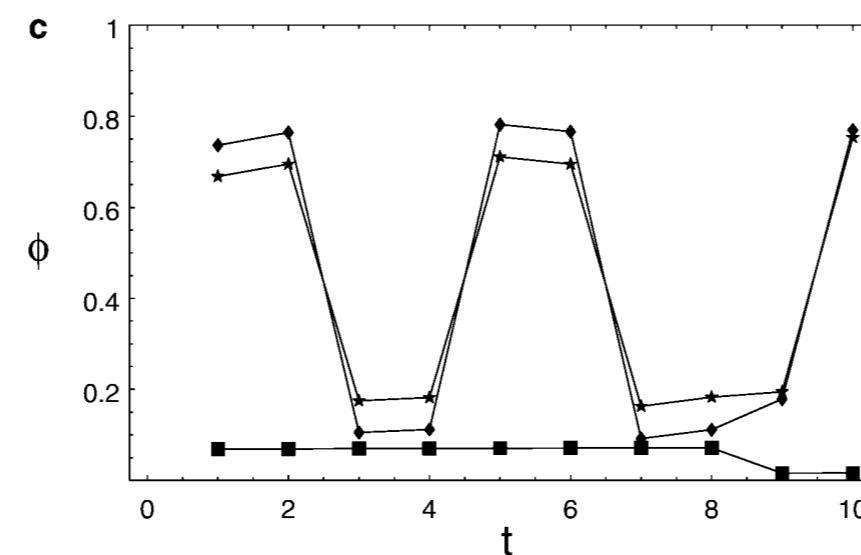
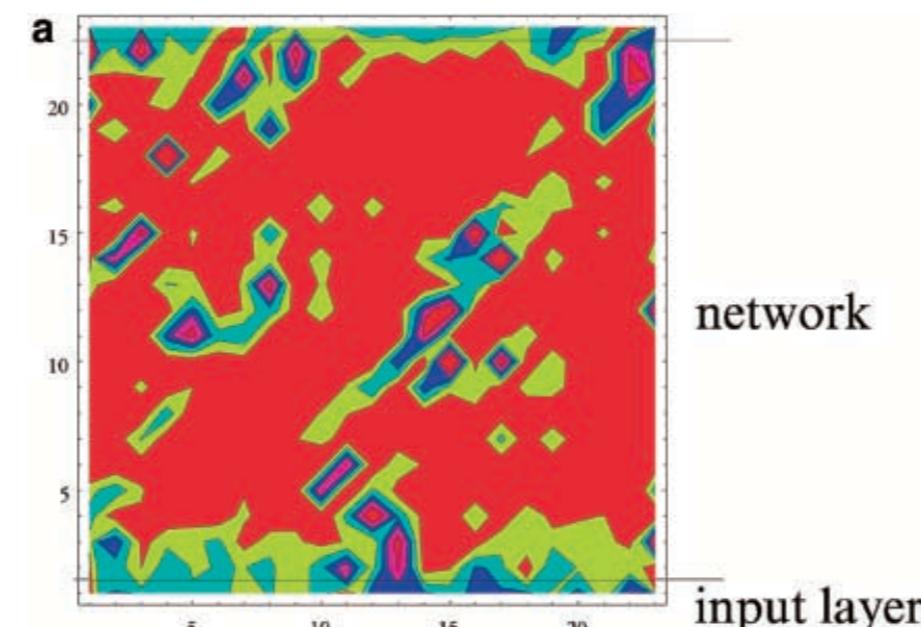
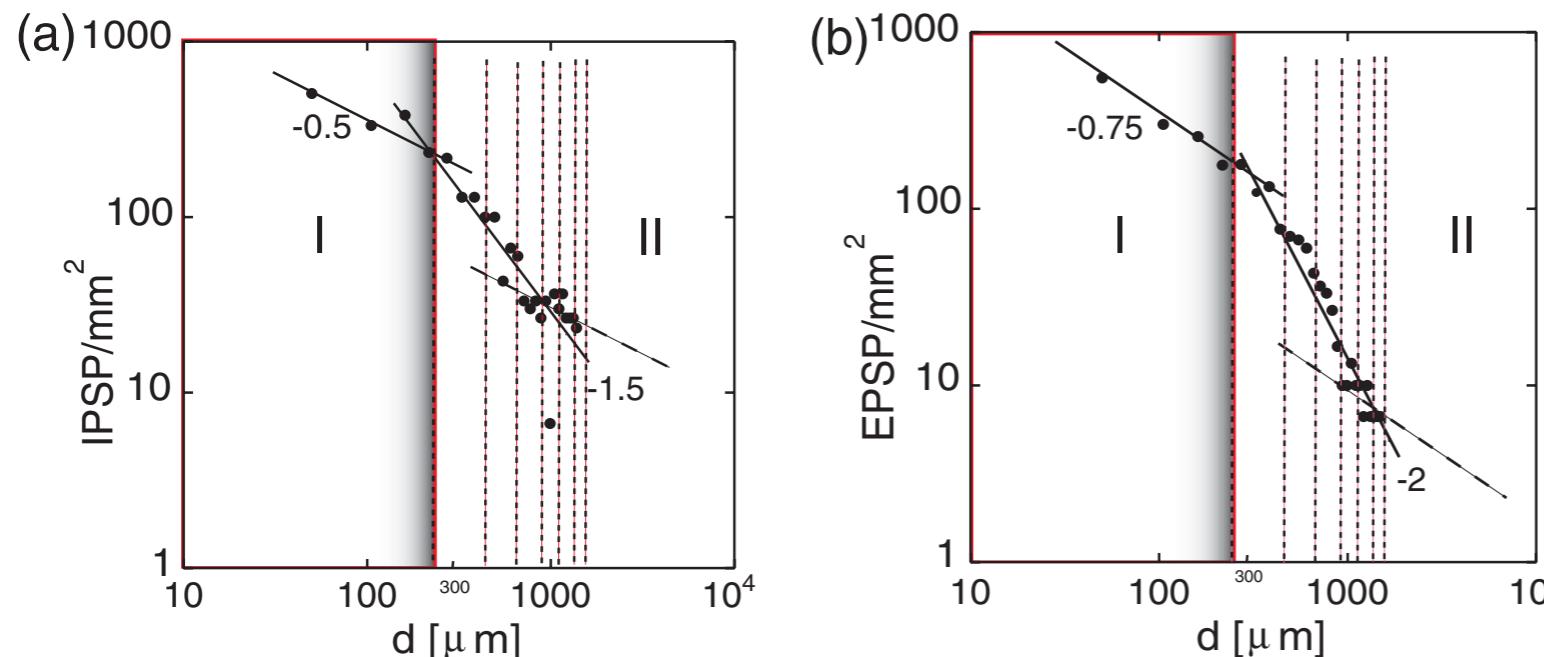


Fig. 8. **a** Phase differences evoked by two distinct input patterns (2-d network, evolution under phase-coincidence detection). In the *red area*, no changes are observed. The *bottom layer* (=input layer) shows the differences in the input patterns. Due to two-torus periodic boundary conditions, this also affects the top layer. Coding sites are the islands within the red sea. At these sites, prominent phase changes are observed. **b** Corresponding figure when excitatory phase return maps have extended refractory periods. A visibly increased “penetration depth” of coding sites indicates increased degree of synchronization. **c** Temporal phase difference evolution, at a coding site from (a). Three input signals were compared (constant random phase layer l_1 , constant layer l_2 with phase 0.2, constant layer l_3 with phase 0.6). Absolute phase differences are shown of, *top curve*: $l_1 - l_2$, *medium curve*: $l_1 - l_3$, *bottom curve*: $l_2 - l_3$.

Next level: What's in cortical columns?

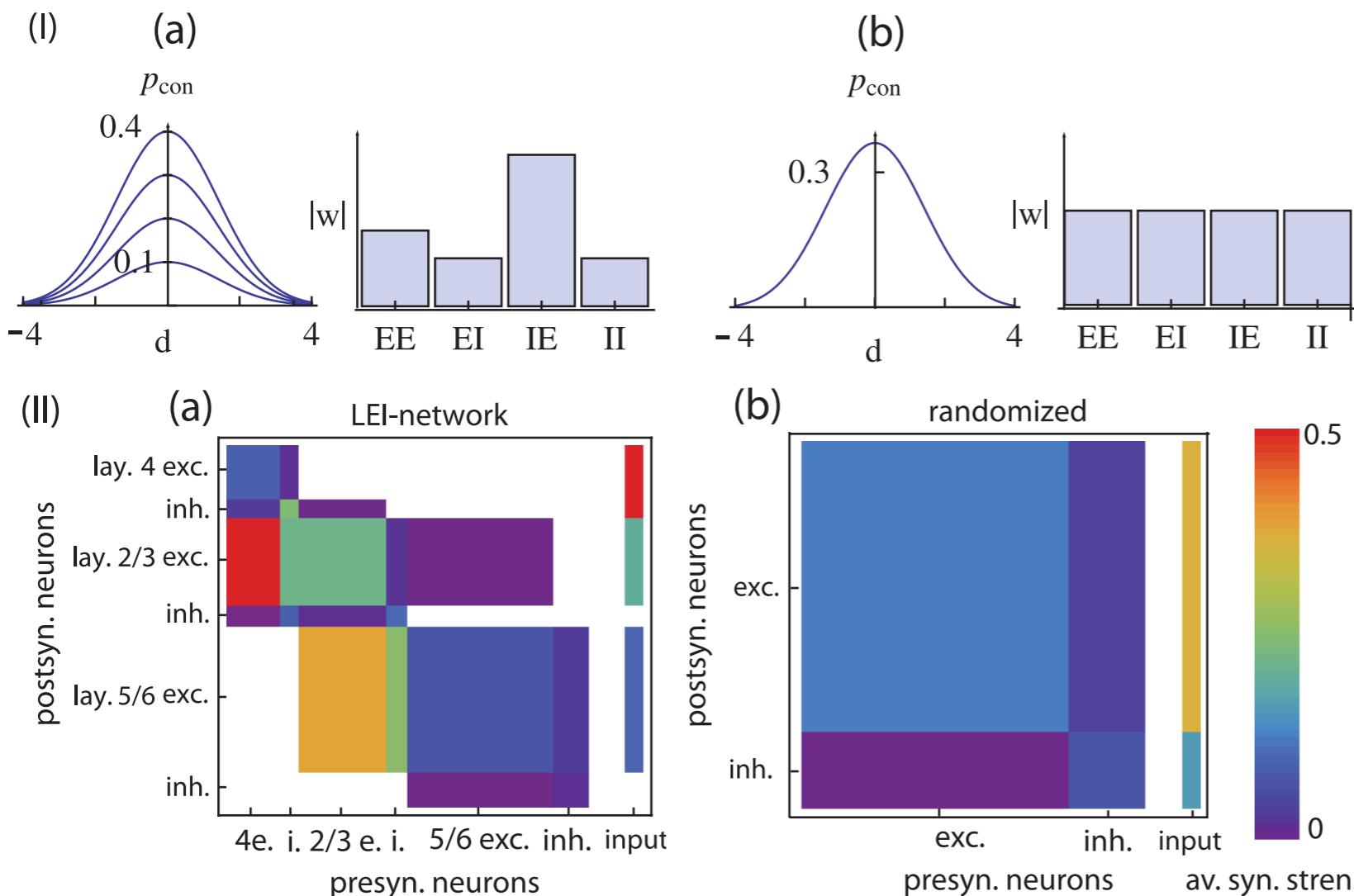


double power-law!

Log-density of photostimulation—evoked excitatory (a) and inhibitory (b) synaptic inputs (concentric rings 50 μm apart, from 19 pooled layer 2/3 neurons). (I): Inner-columnar, (II): Intercolumnar scale. Vertical lines: Extensions of aligned physiological columns. Tilted dashed lines: Proposed long distance decay.

B. Roerig and B. Chen, *Cereb. Cortex* **12**, 187 (2002).

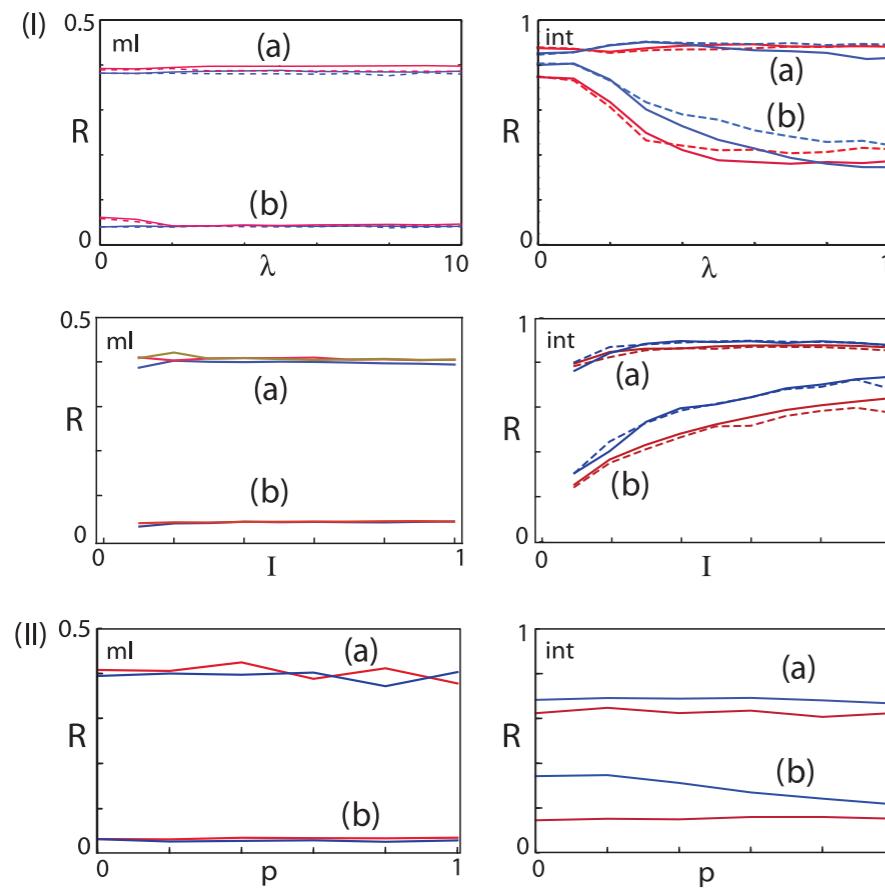
Testing the ‘canonical microcircuit’ dogma



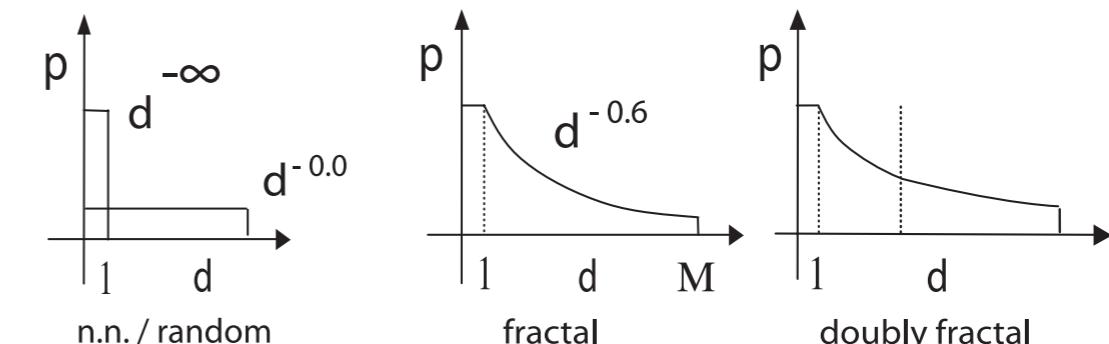
(I) (a) EI model, (b) EI-control network (uniform synaptic weights w , $\lambda = 2$). p_{con} : probability of a synaptic connection among neurons of distance d for C values as in the text, w : synaptic strength of the connections. (II) (a) LEI-model, (b) LEI-control network. Input strengths to populations are color coded.

‘reservoir computing’

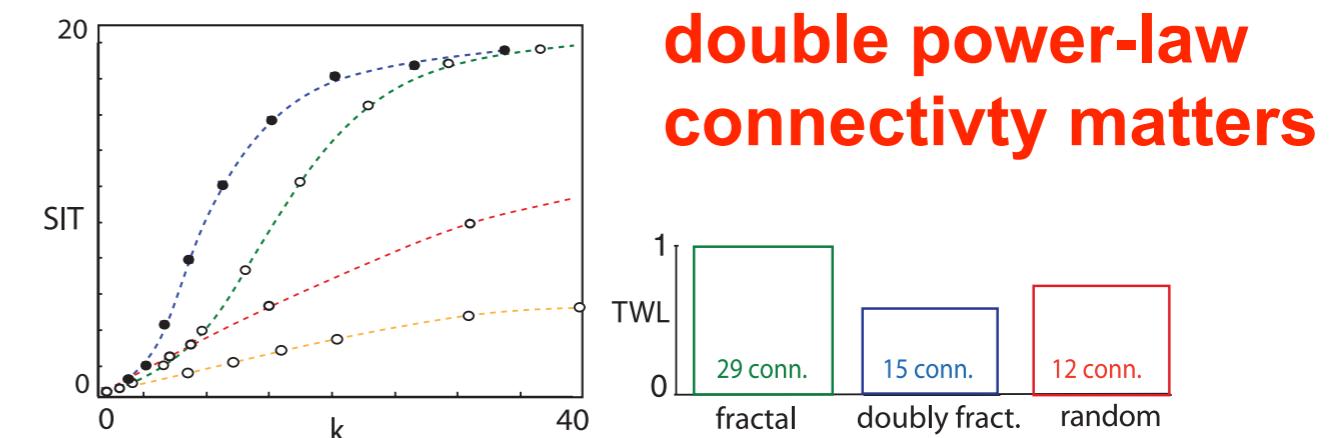
Columnar wiring does not matter, except for..



Recognition rate R for (a) Arabic Digit, and (b) Auslan recognition. Each data point represents an average over at least 20 experiments following a normal-like distribution each [cf. Supplemental Material Sec. (1b) [10]]. Blue: leaky integrate and fire, red: Izhikevich neurons. Left column: memoryless (ml), right column: integration (int) readout. (I) *EI* network, dependence on rewiring parameter λ (control networks: dashed curves), and on ratio I of input receiving neurons, at local connectivity (i.e., $\lambda = 2$). Ocher: Izhikevich neurons with $\lambda = 0$. (II) *LEI* networks, dependence on rewiring probability p . $p = 0$: layered, $p = 1$: homogeneous control network.



Main connectivity classes compared (p : connection probabilities, d : distance, M : cutoff, see text).

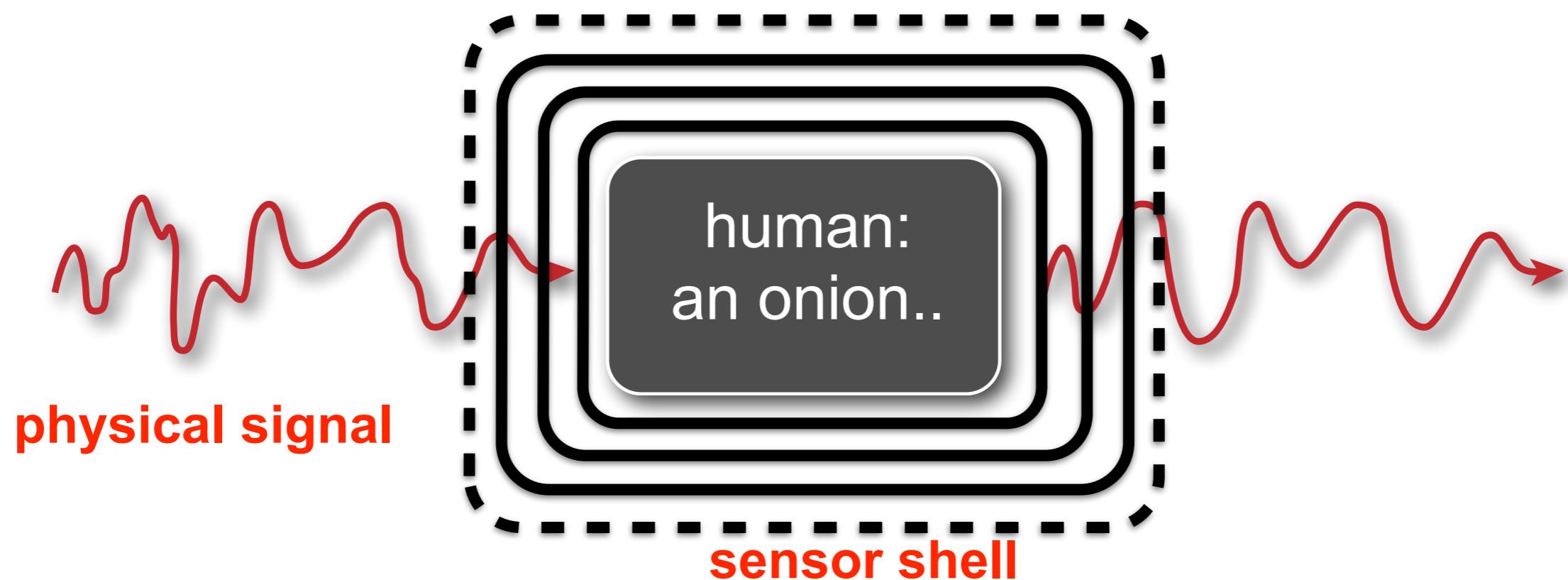


Left: SIT as a function of cell connections k . From top: doubly fractal ($\theta = 0.2$, $\alpha = 0.5$, $\beta = 2.0$), fractal ($\theta = 1$, $\alpha = 0.7$), random, n.-n. topology. Network sizes: $N = 4096$, averages over 100 experiments. Right: Connections k_{min} required for synchronization, and associated TWL. $N = 512$, 10 experiments.

Follow the money... Change of approach: 'explain the brain'!



- > follow the information flow



Hearing system properties:

- Ancestral to the nervous system
(hope: explain aspects of the brain from the sensors' perspective)
- Verifiable ('big' unexplained data)
- Simple fundamental physics-based model
- Powerful if embedded into physiological context
- Explains a number of puzzling observations



Overview:

- 1995: Wiesenfeld: Small signal amplifiers, PRL
- 1999: Start: Kern-Stoop cochlea, from scratch, based on fluid dynamics, energy-based approach
- 2000: Eguiluz, PRL: Hopf concept
- 2002: Kern's thesis finished
- 2003: Kern & Stoop, PRL
- 2003: Comment to Magnasco's PRL
- 2004: Stoop & Kern, PRL, PNAS
- 2004: Efferent tuning, submitted to SNF
- 2005: Coupling reconsidered, v.d.Vyver
- 2005: Hardware cochlea, v.d.Vyver
- 2006: v.d.Vyver's thesis, ETHZ
- 2006: US Patent filed
- 2006: Insect hearing: Hopf in Drosophila antenna
- 2008: Cochlear re-mapping
- 2010: Local correlations of the perceived pitch, PRL
- 2011: Effect of Nuclei, NECO
- 2013: Pitch sensation involves stochastic resonance, Sci. Rep.
- 2014: Efferent tuning implements listening, Phys. Rev. Appl.
- 2014: Pitch sensation shaped by cochlear fluid, Nat. Phys.
- 2016: Signal-coupled subthreshold Hopf-type systems show sharpened collective response, PRL
- 2016: Auditory power-law activation avalanches exhibit a fundamental computational ground state, PRL
- 2017: Mammalian hearing threshold explained, Sci. Rep.
- 2018: "Harmony" perception explained from network principles

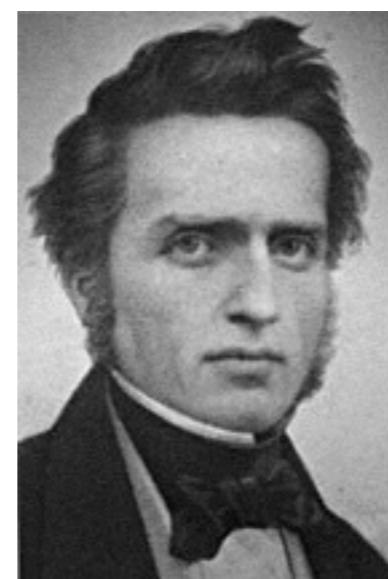


Q: What do we hear and why?

1840: Berlin vs. Dresden



Ohm



Seebek

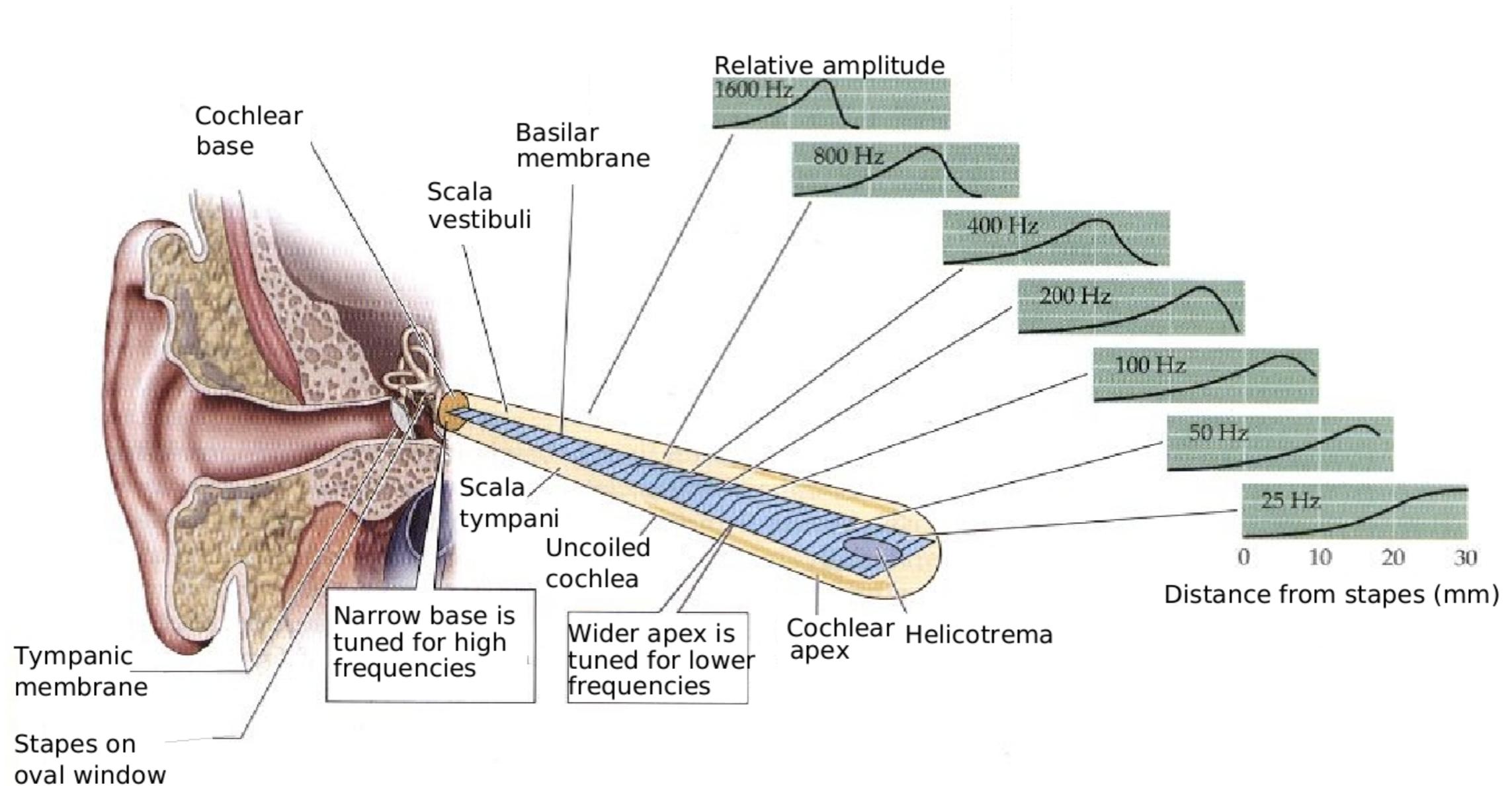
**What is the physical description
of ‘pitch’ sensation?**

“Wodurch kann über die Frage, was zu einem Tone gehöre, entschieden werden, als eben durch das Ohr?”
(How else can the question as to what makes out a tone, be decided but by the ear?)

August Seebeck 1844

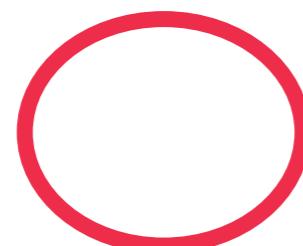
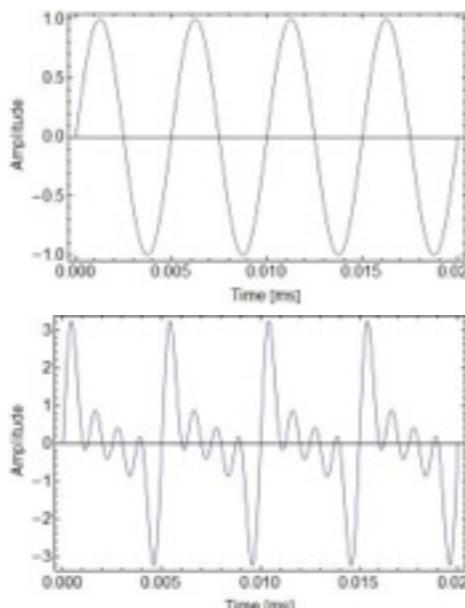
Mammalian cochlea

more than a frequency analyzer..

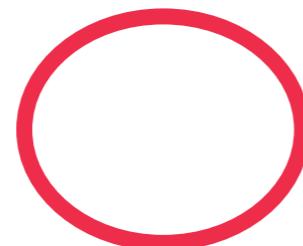


Experiments

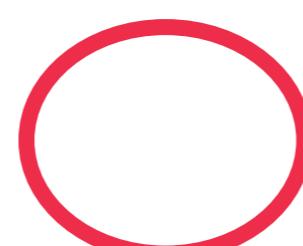
- simple tone: $A \cdot \sin(2\pi f_0 t)$
- complex tone:
(frequency components
 $f_0, 2f_0, 3f_0, \dots$)
- missing fundamental



simple

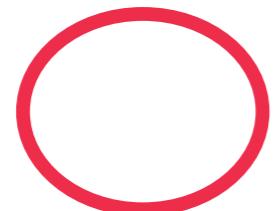
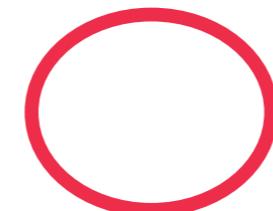


complex



missing fundamental

- Smoorenburg's two-tone experiments:

1750/2000 \rightarrow 1800/2000 Hz

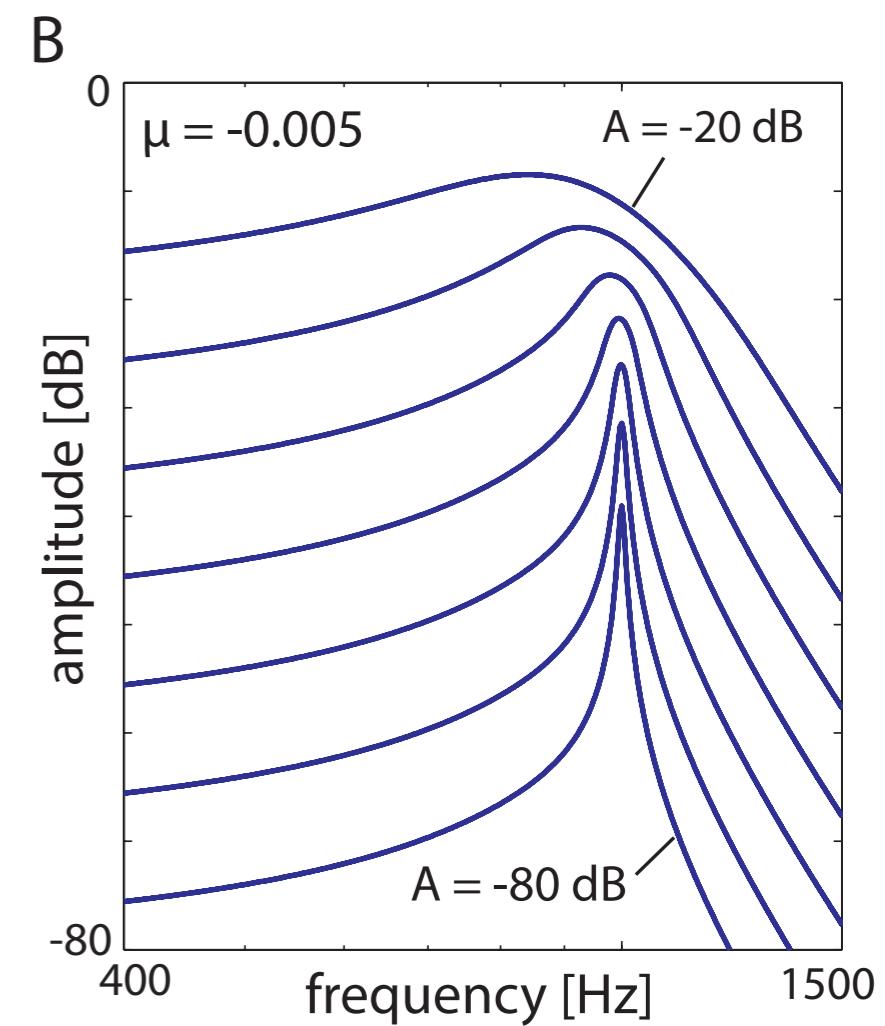
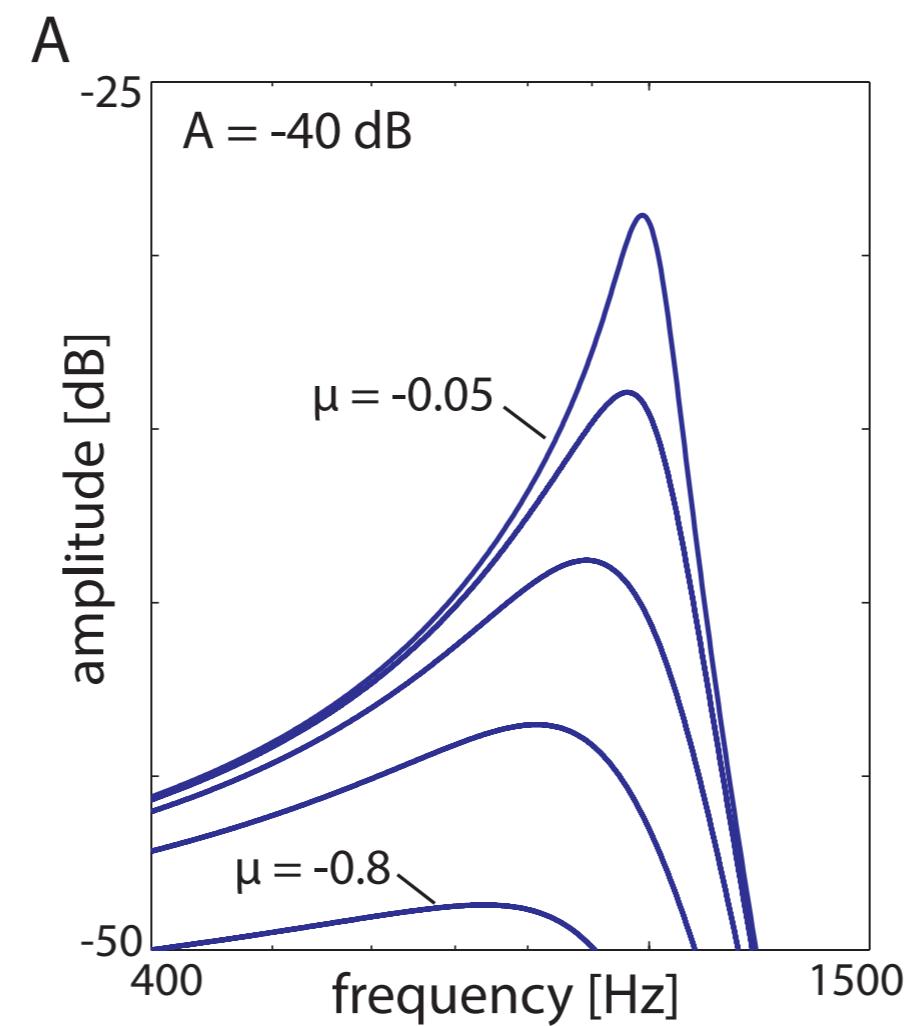
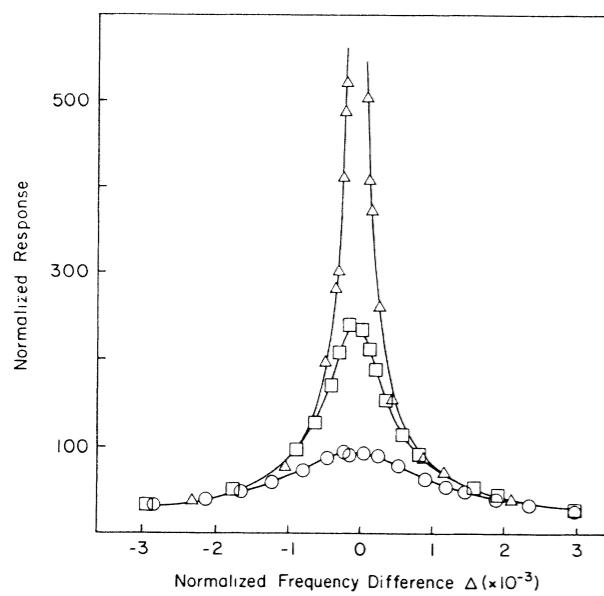
reversed

pitch down (250 \rightarrow 200 Hz, fundamental), or pitch up ?

I Key for understanding hearing: nonlinear 'small signal amplifier'

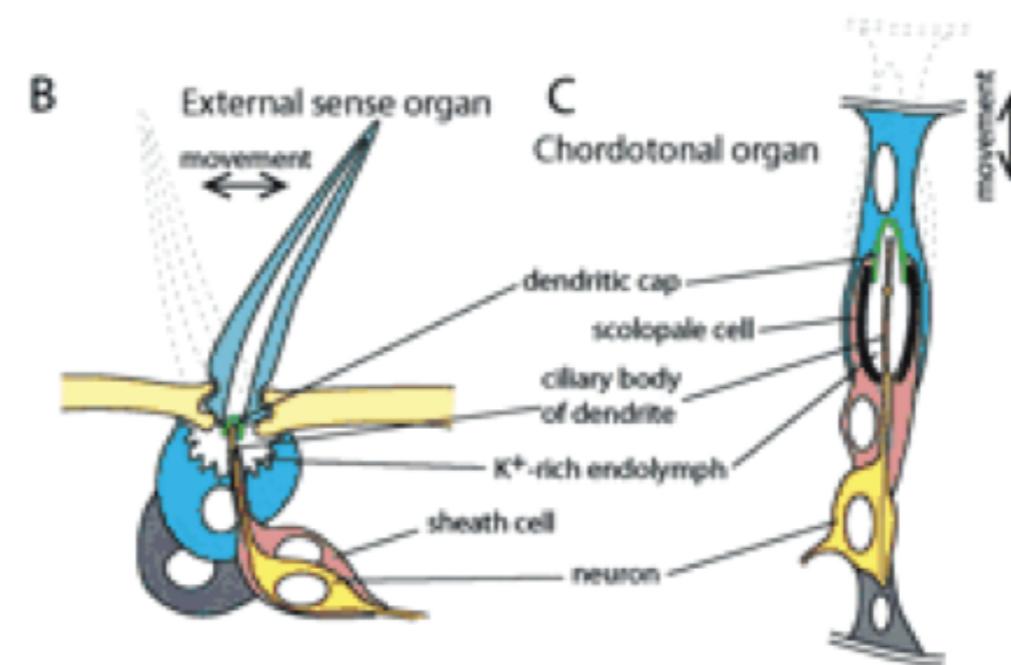
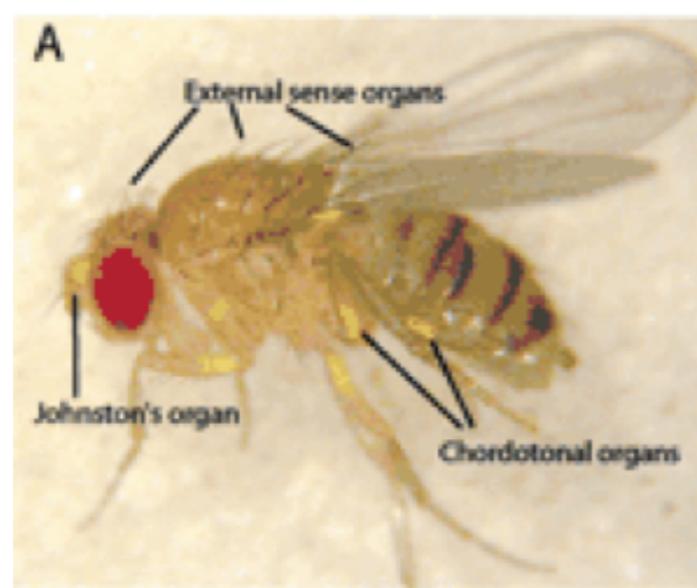
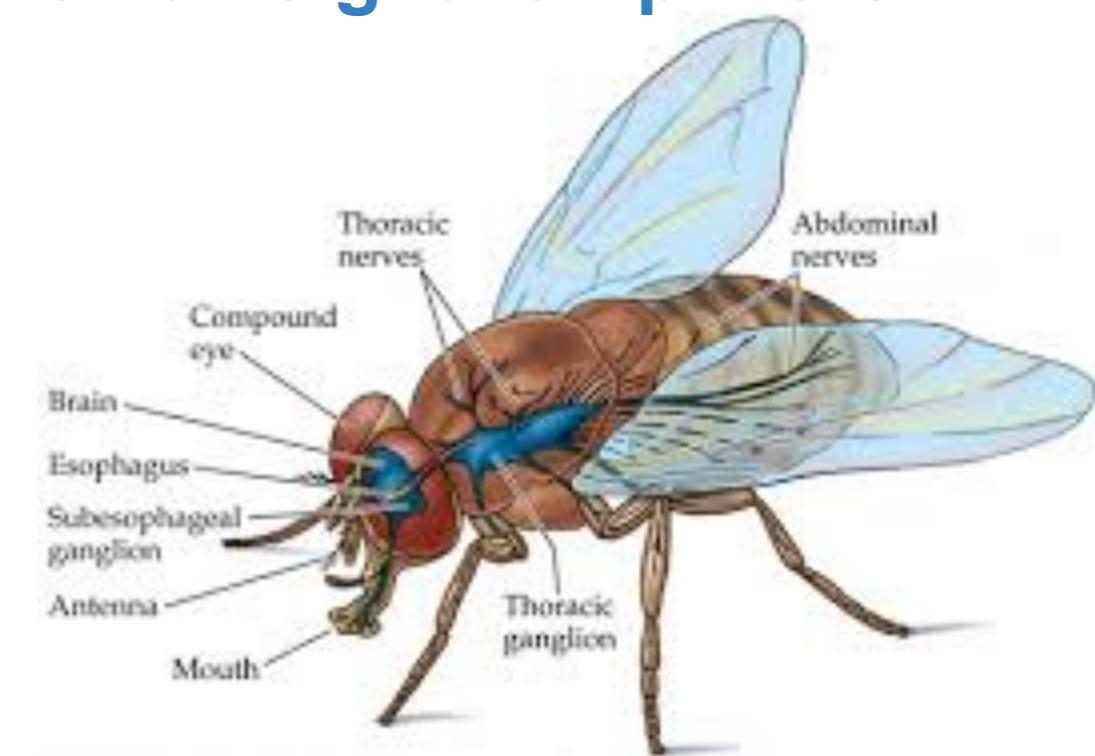
Wiesenfeld et al. PRL 1984/5/6:

Systems close to a **period-doubling bifurcation** can be used as a small signal amplifier:
Signals with a certain 'critical' frequency are strongly amplified.



Andronov-Hopf: Brun et al., PRL 1985

Biological evidence of Hopf small signal amplifiers

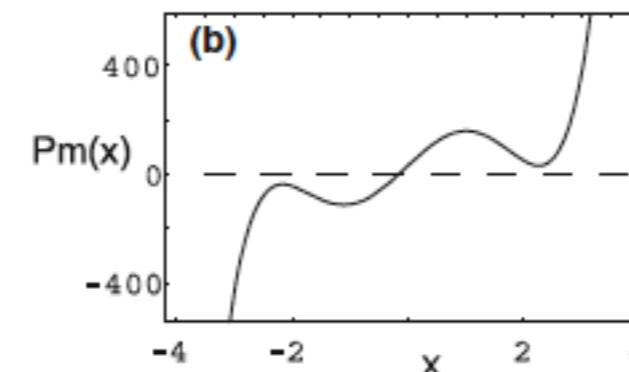
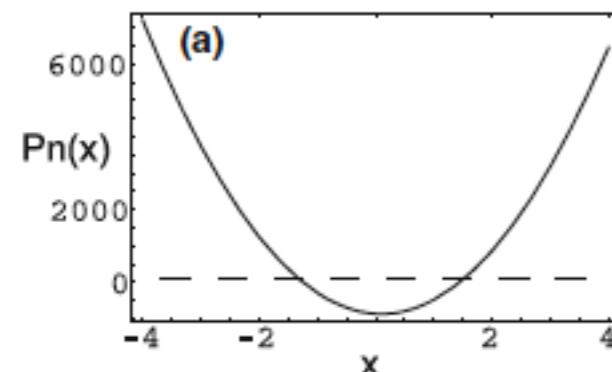


Dynamics above bifurcation demonstrate the Hopf property

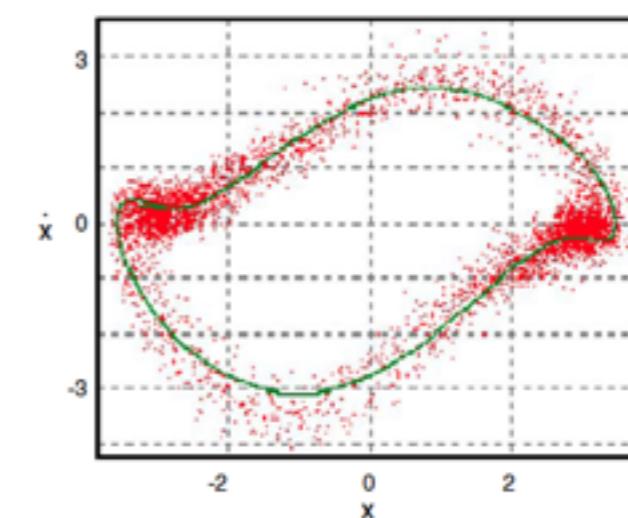
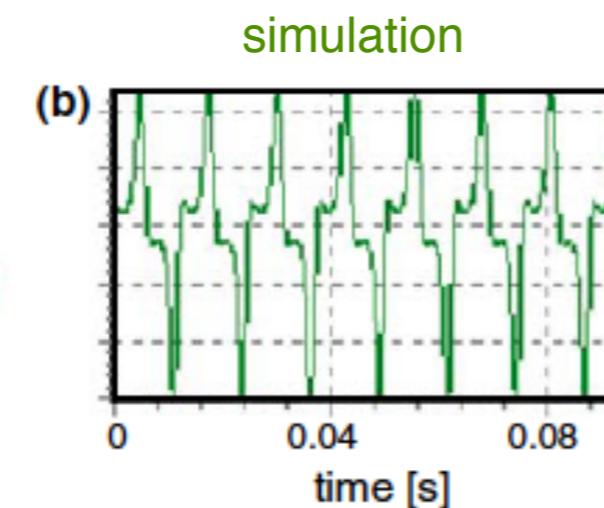
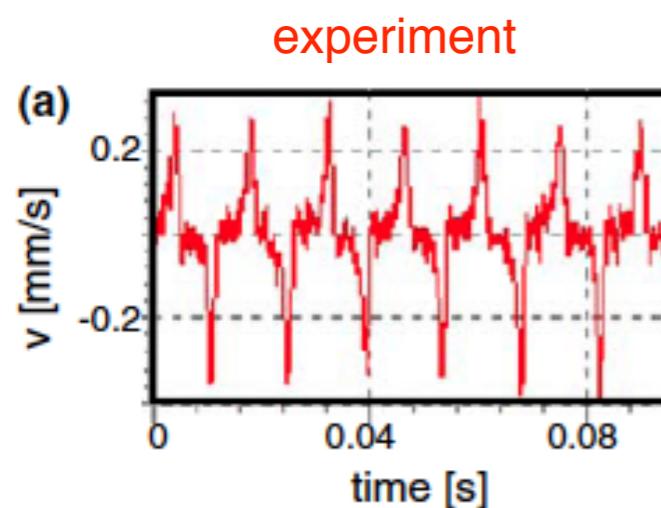
$$\ddot{x} + P_n(x)\dot{x} + P_m(x) = 0$$

$$\ddot{x} - \mu(1 - x^2)\dot{x} + x = 0$$

Generalized van der Pol oscillator
 $\mu=0$: A.-Hopf bifurcation



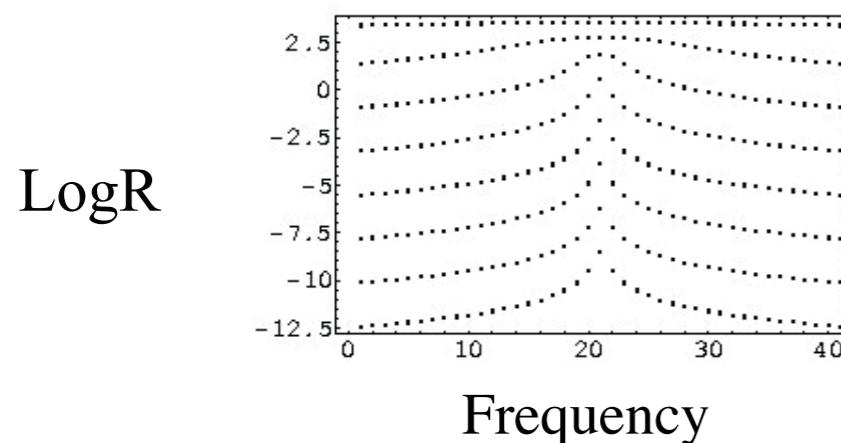
$P'm(x)$, restoring force, negative stiffness
 $(P'm(x)<0$: active amplification)



R.S. et al, Eur. Biophys. J. 2006
 T.L., F.G. & R.S. Sci. Rep. 2015

Active response R from a forced Hopf system (F: forcing)

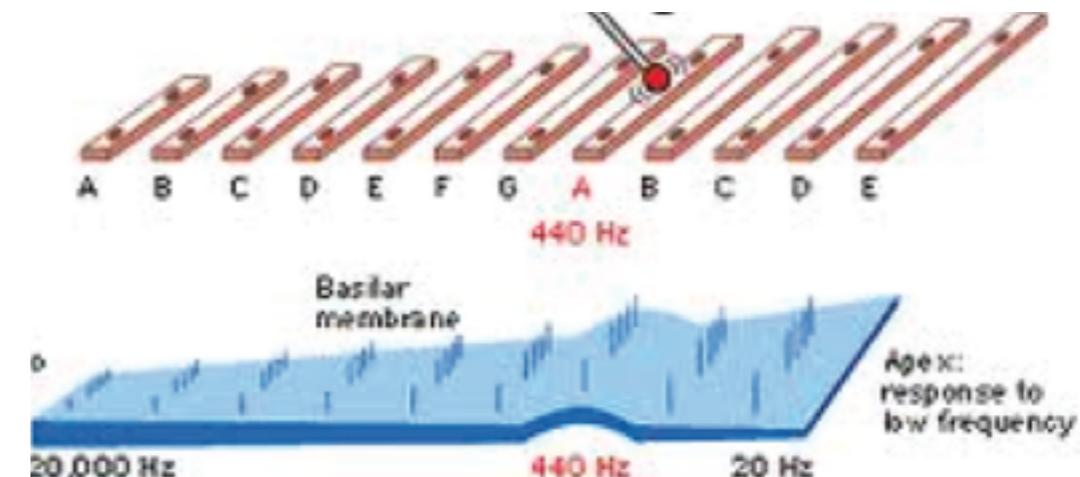
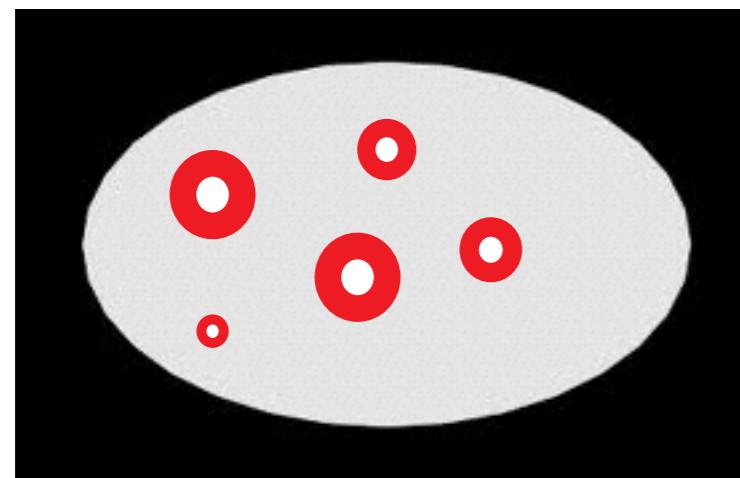
- Close to bifurcation point and resonance: $R = F^{1/3}$
- Before bifurcation point, small F : $R = -F/\mu$
- Charakteristic of Hopf-bifurcation



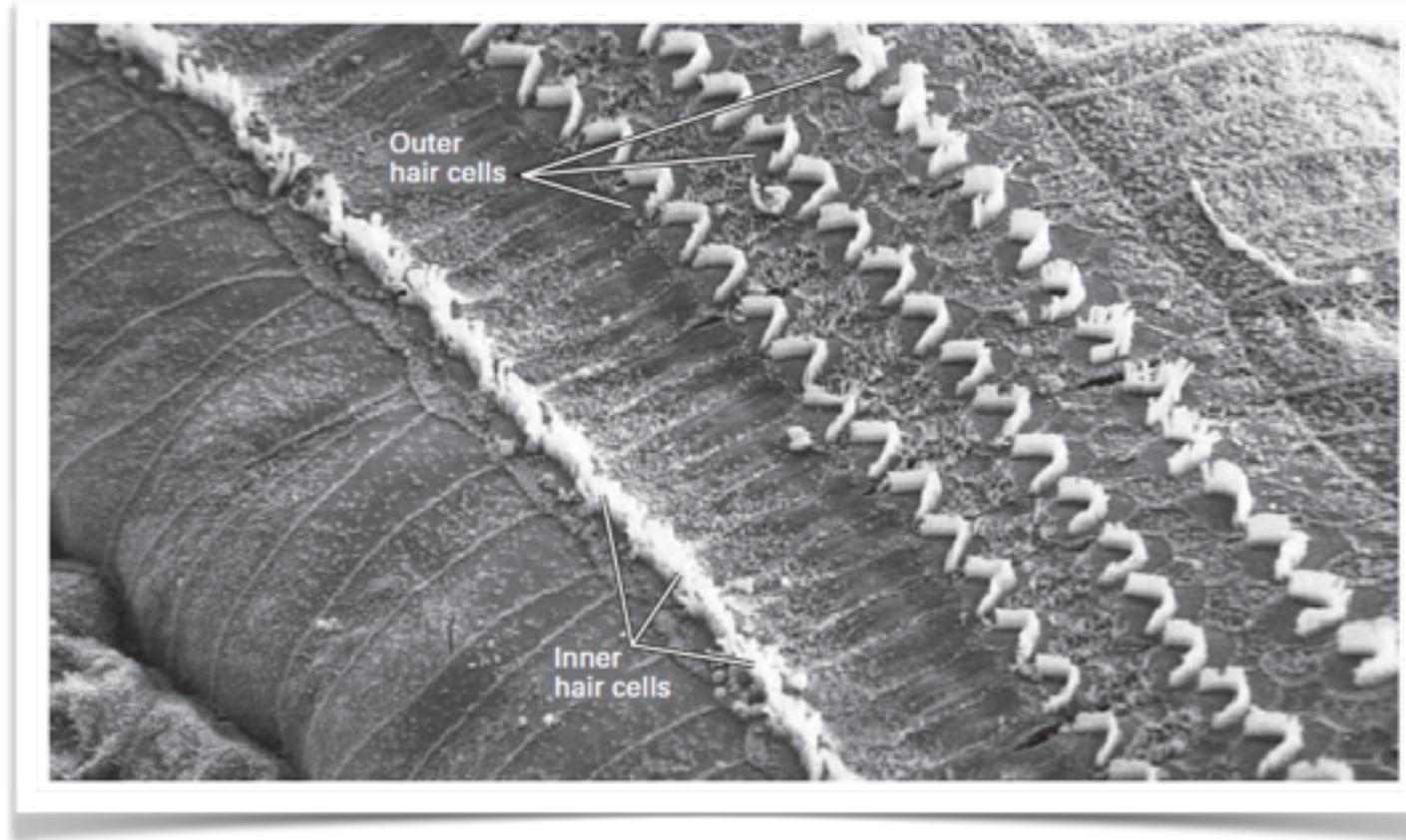
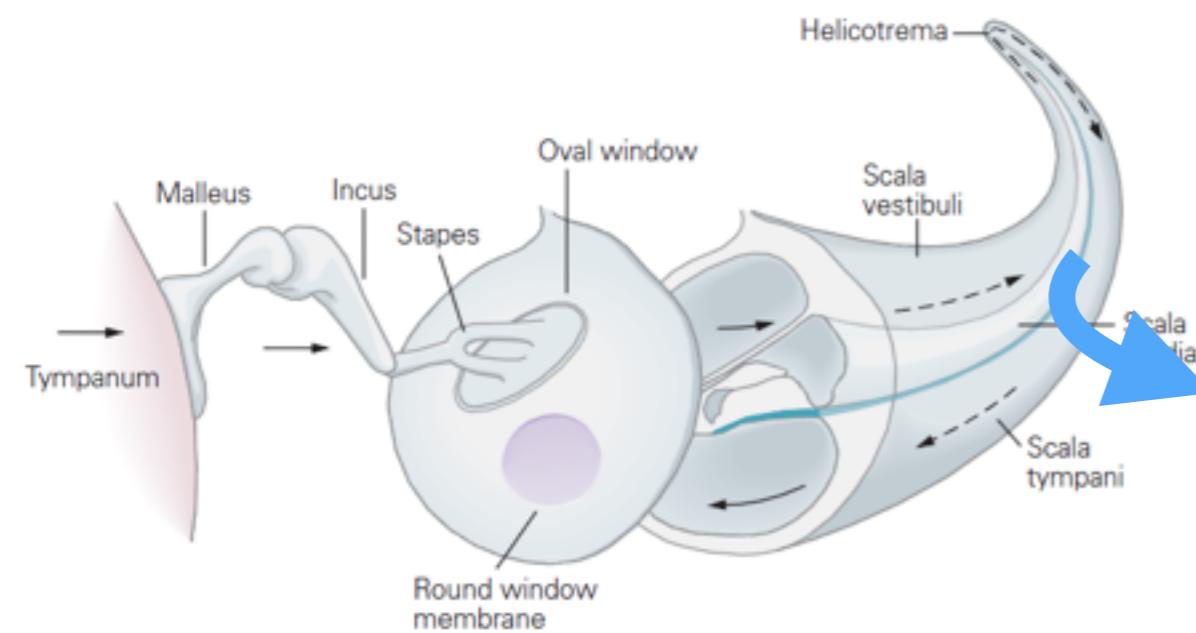
$w_c = 1000 \text{ Hz}$, $\mu = -20$, governs G
 $F = \{0.004 \cdot 10^i, i=0..7\}$

(Eguiluz et al. PRL 2000)

II From many sensors to a cochlea: the wiring problem

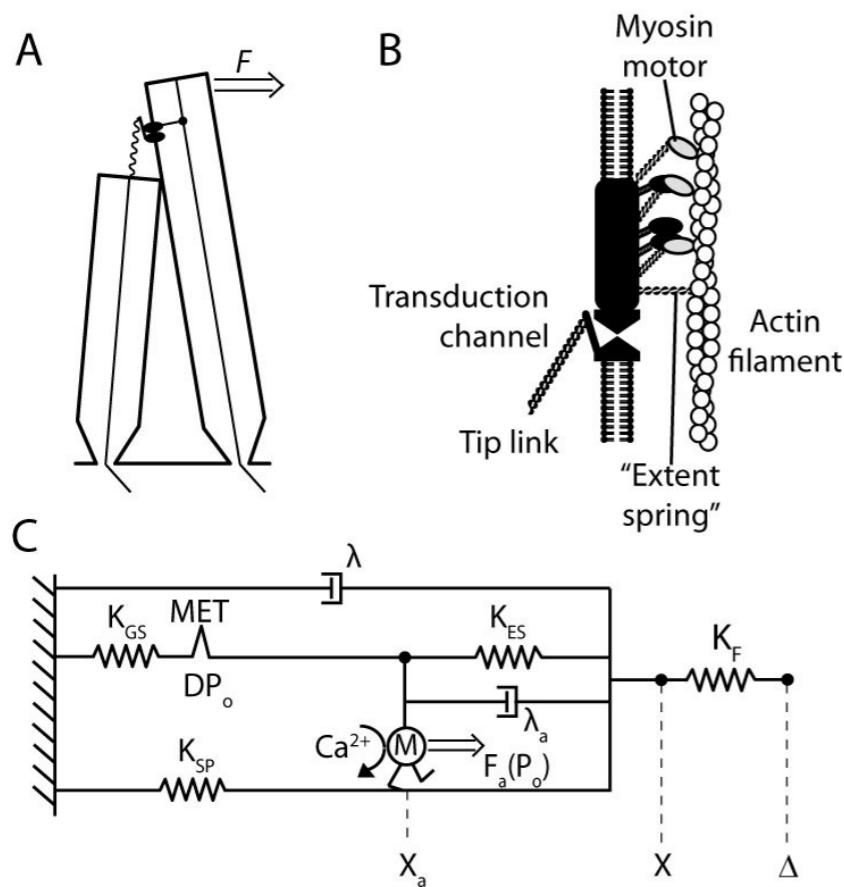


(Lorimer, Gomez, R.S., Sci. Rep. 2015)



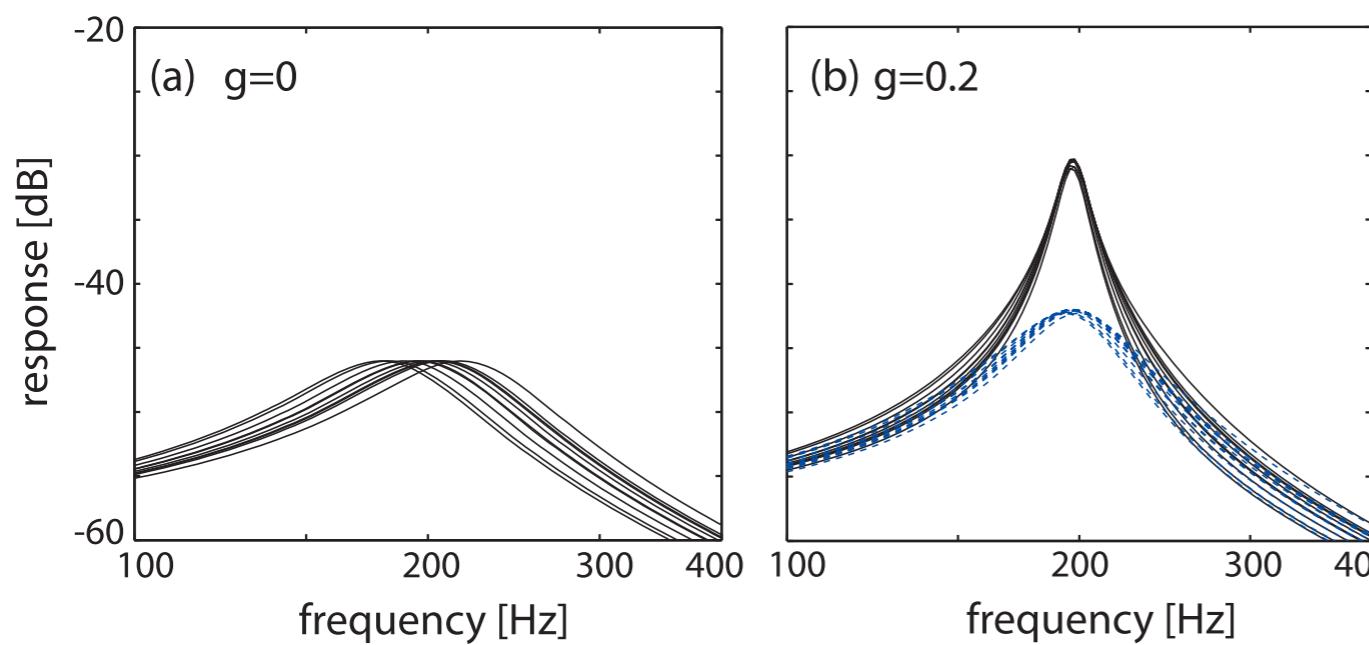
Hudspeth 2013

Generic properties: Individual vs. signal-coupled Hopf elements



$\nu, \rho, m, \text{BM-stiffness} \longrightarrow \mu$

A.K. PhD thesis ETHZ 2003

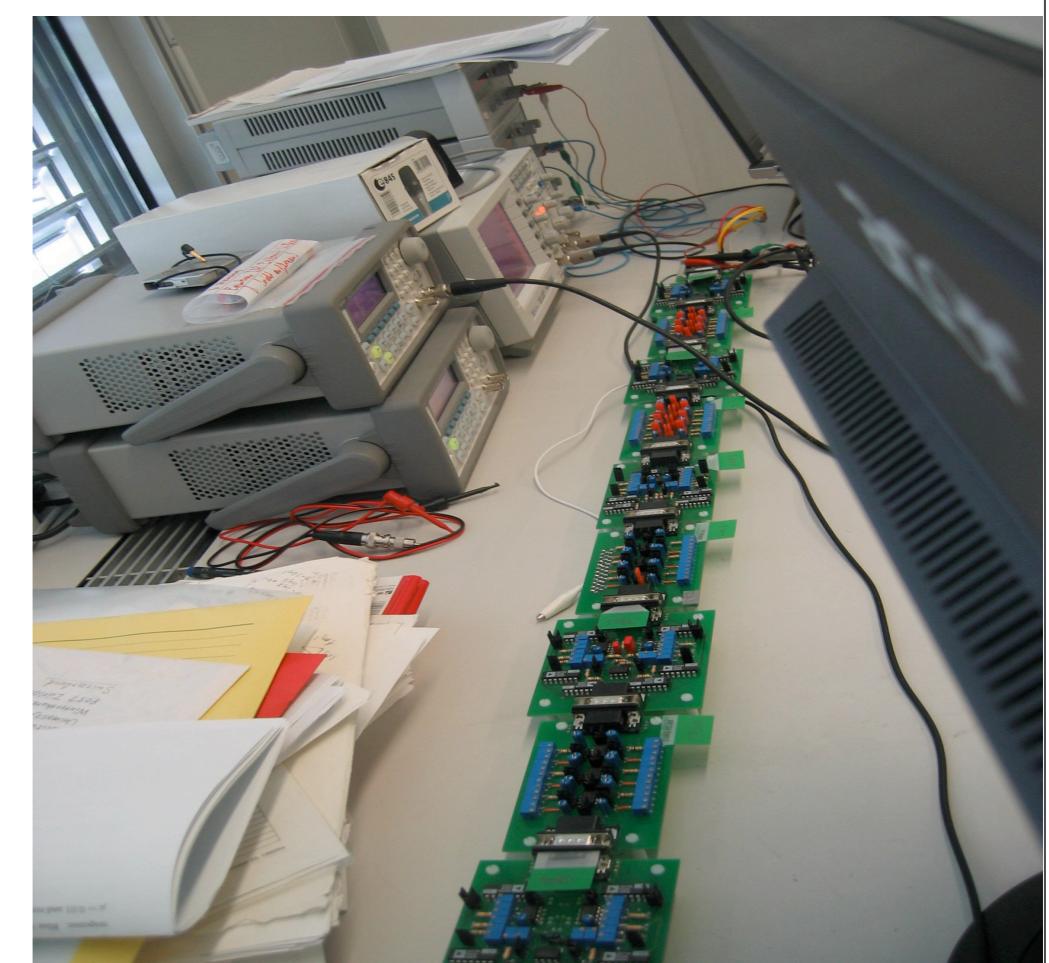
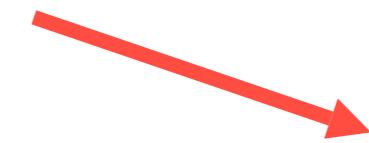
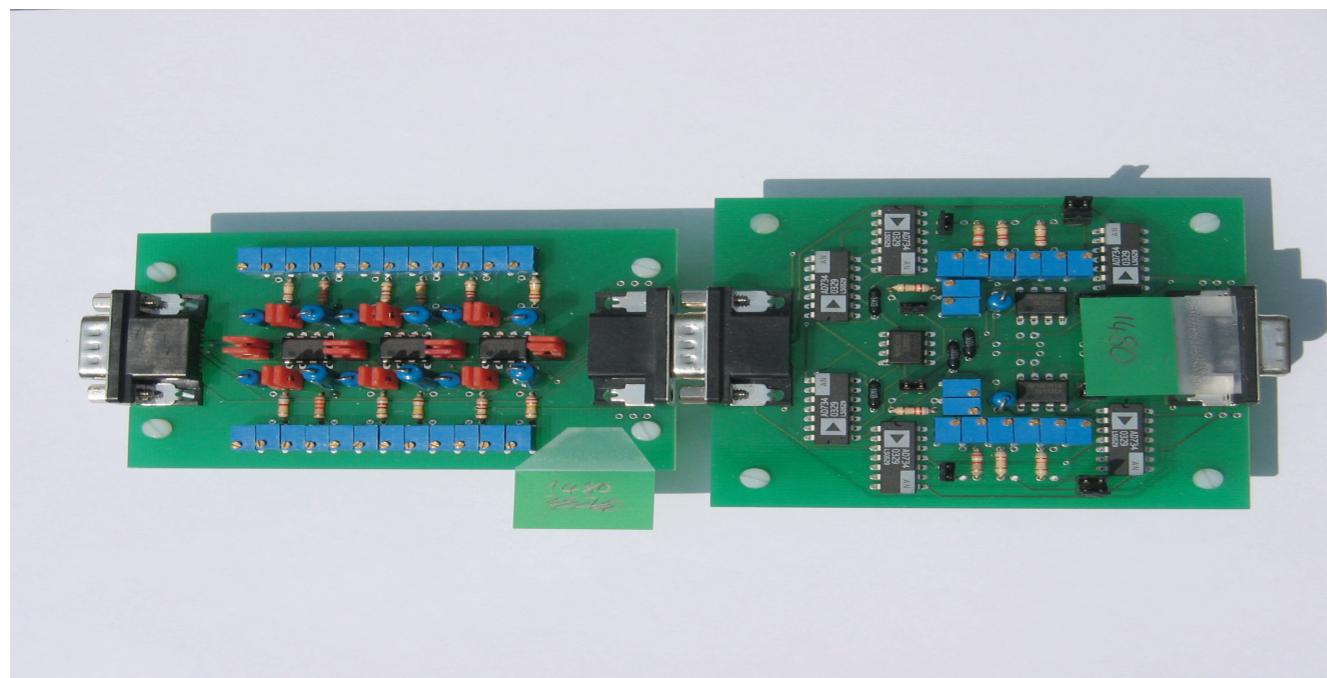


no coupling

signal-coupling: signal sharpening !

F.G, T.L. & R.S. PRL 2016

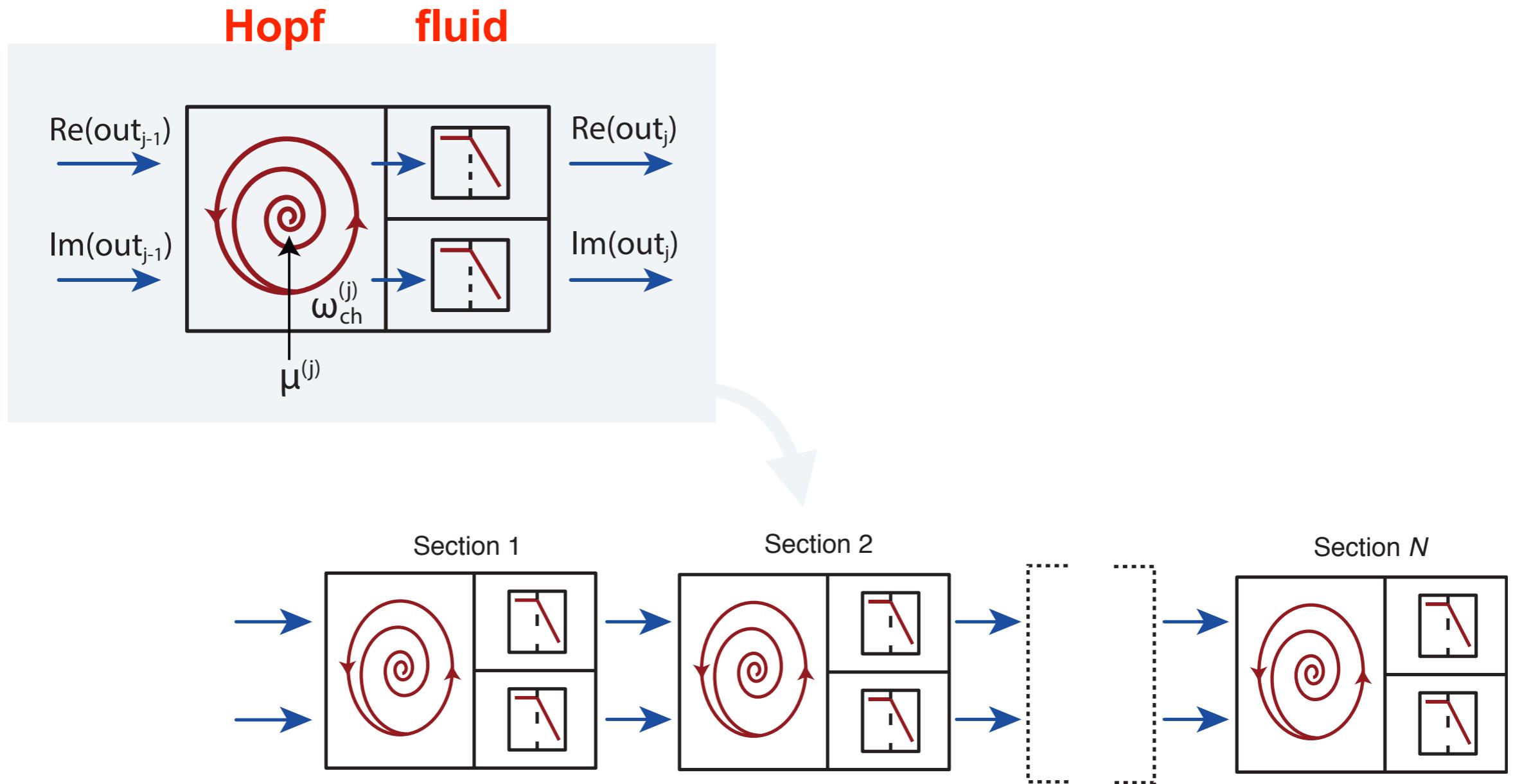
IV Active elements - fluid coupling: Computational simplification



Vyver, Martignoli., R. S. Appl. Phys. Lett. 2008;

US-Patent 2007-2012

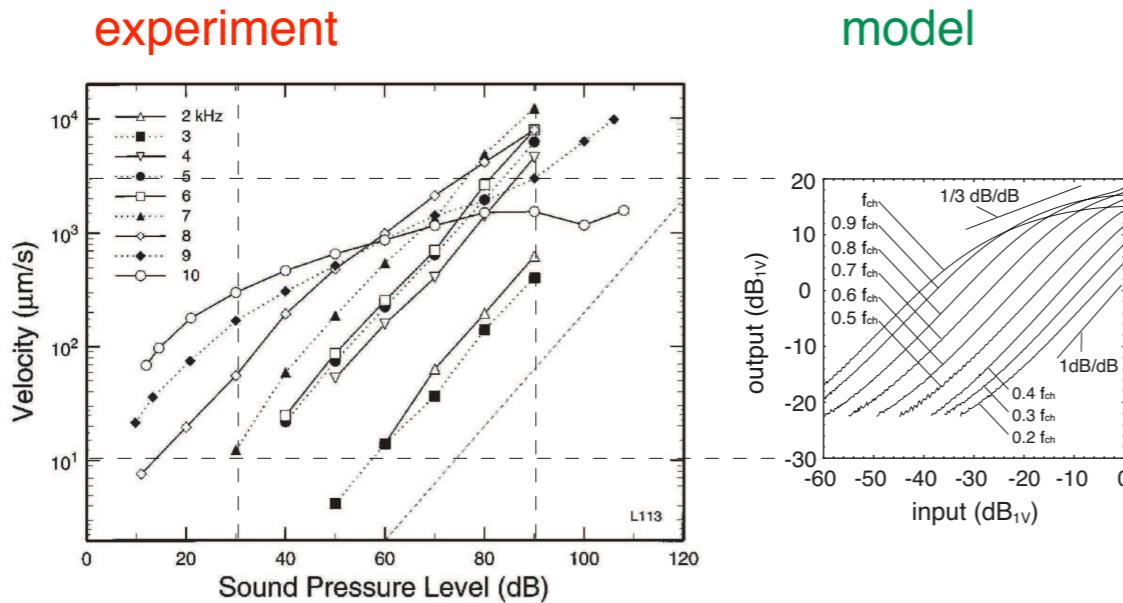
'Hopf cochlea'



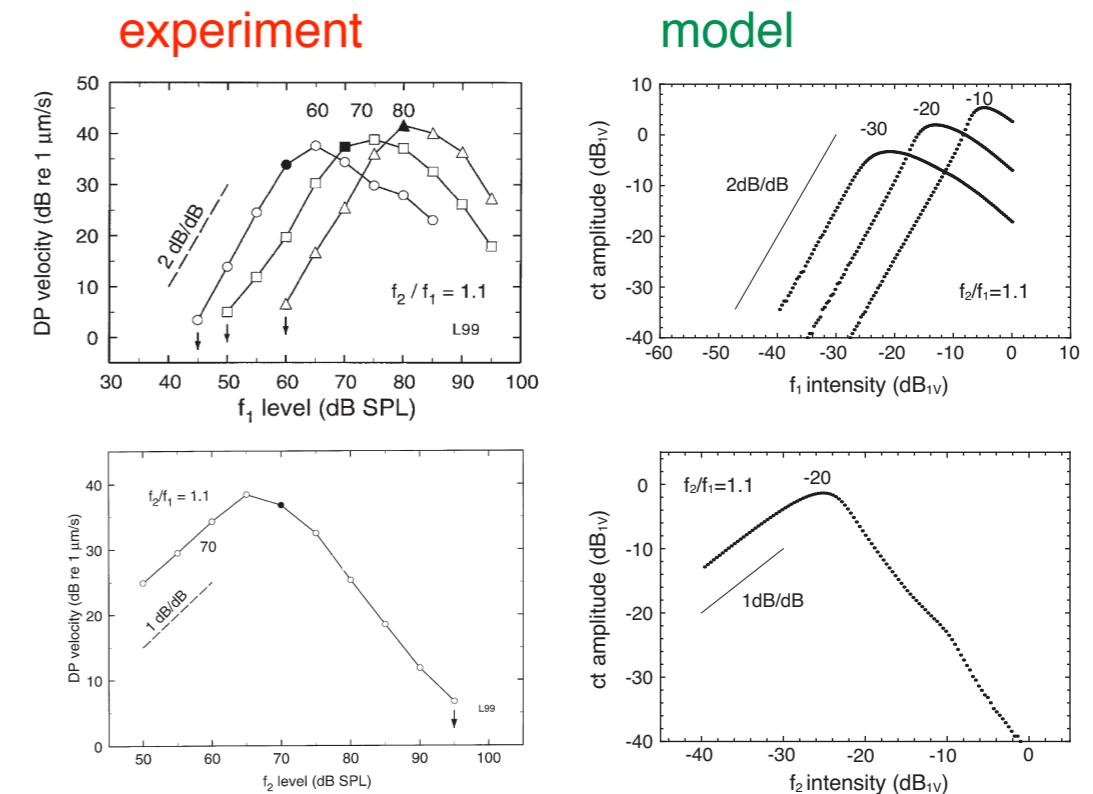
Martignoli, van der Vyver et al. *Appl Phys Lett*, 2007
Martignoli and Stoop *Phys Rev Lett*, 2010
Gomez and Stoop *Nat Phys*, 2014
Stoop and Gomez *Phys Rev Lett*, 2016

Nonlinear phenomena explained:

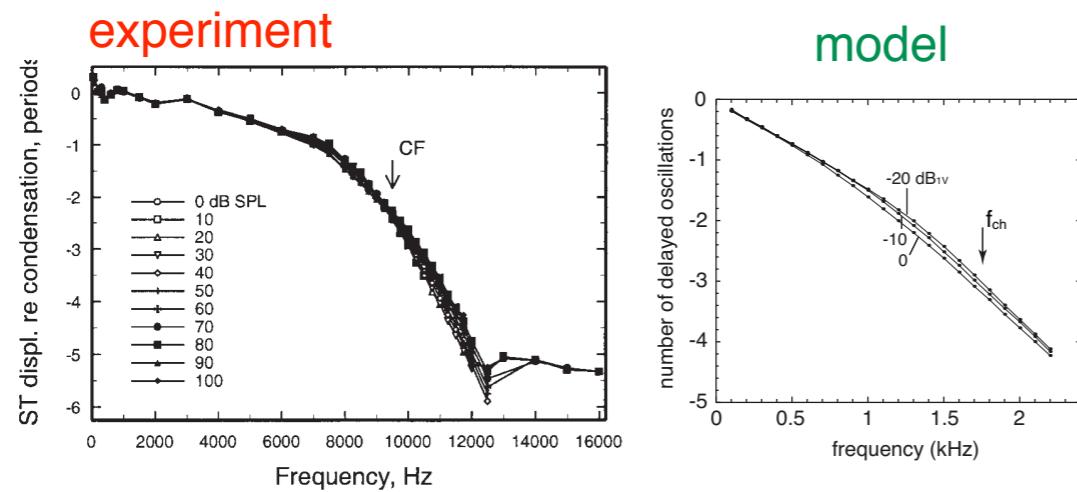
Mutual suppression by two neighboring tones



Combination tones



Phase propagation along cochlea

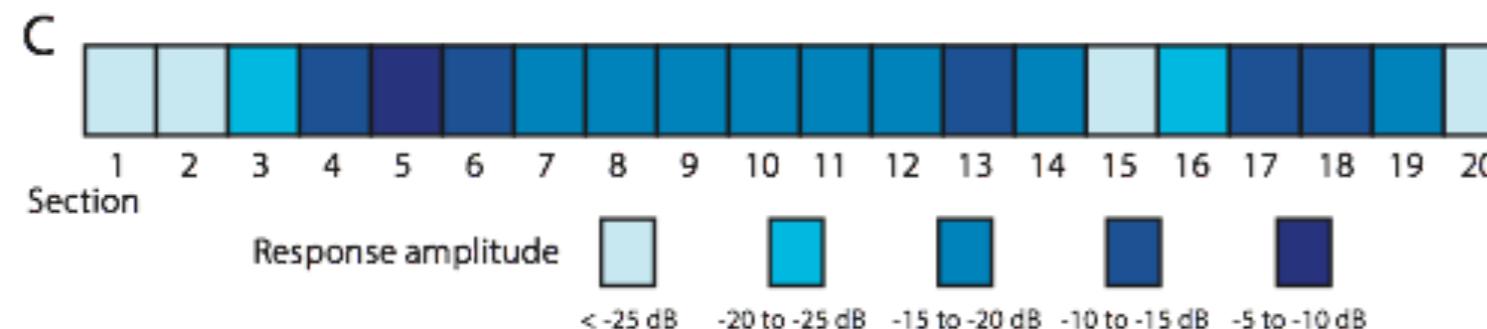
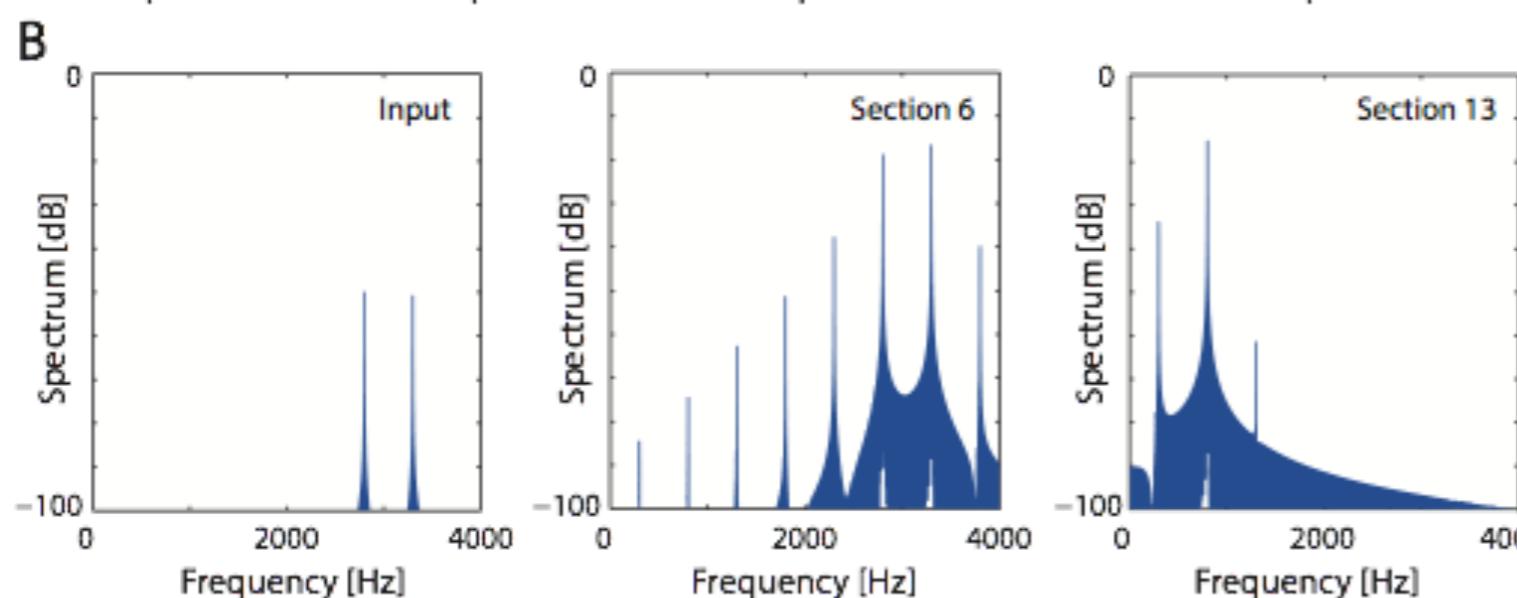
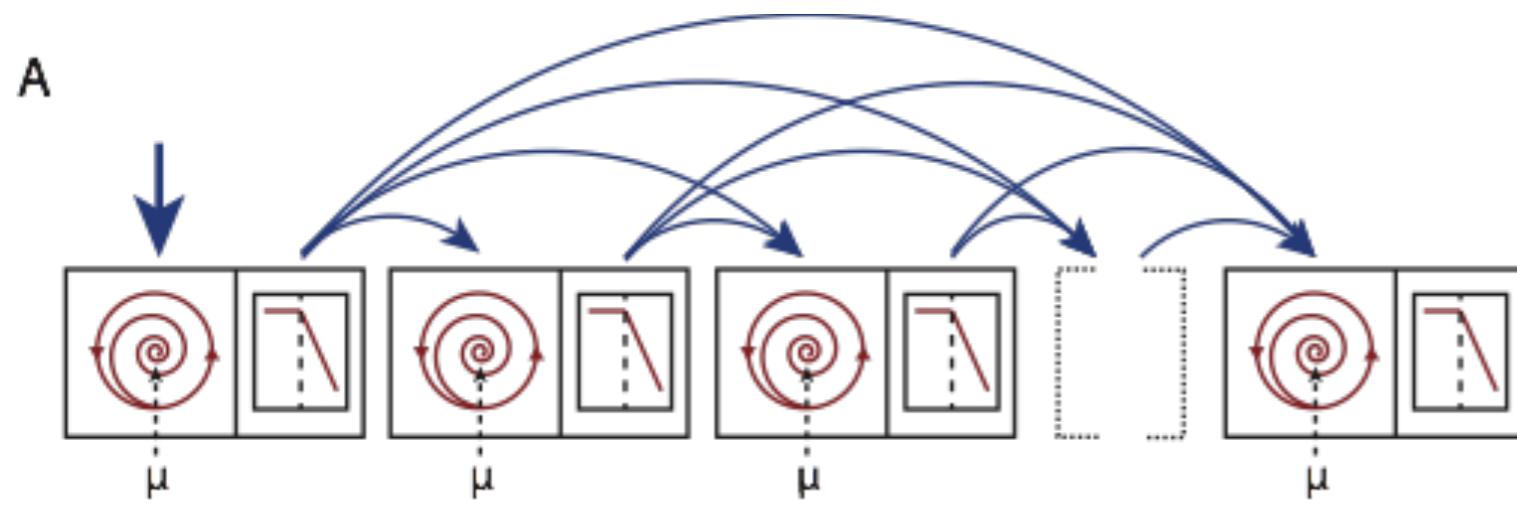


.. and many more, e.g.

Medial olivocochlear efferent stimulation properties

mostly: Stoop and Kern *Phys Rev Lett*, 2004

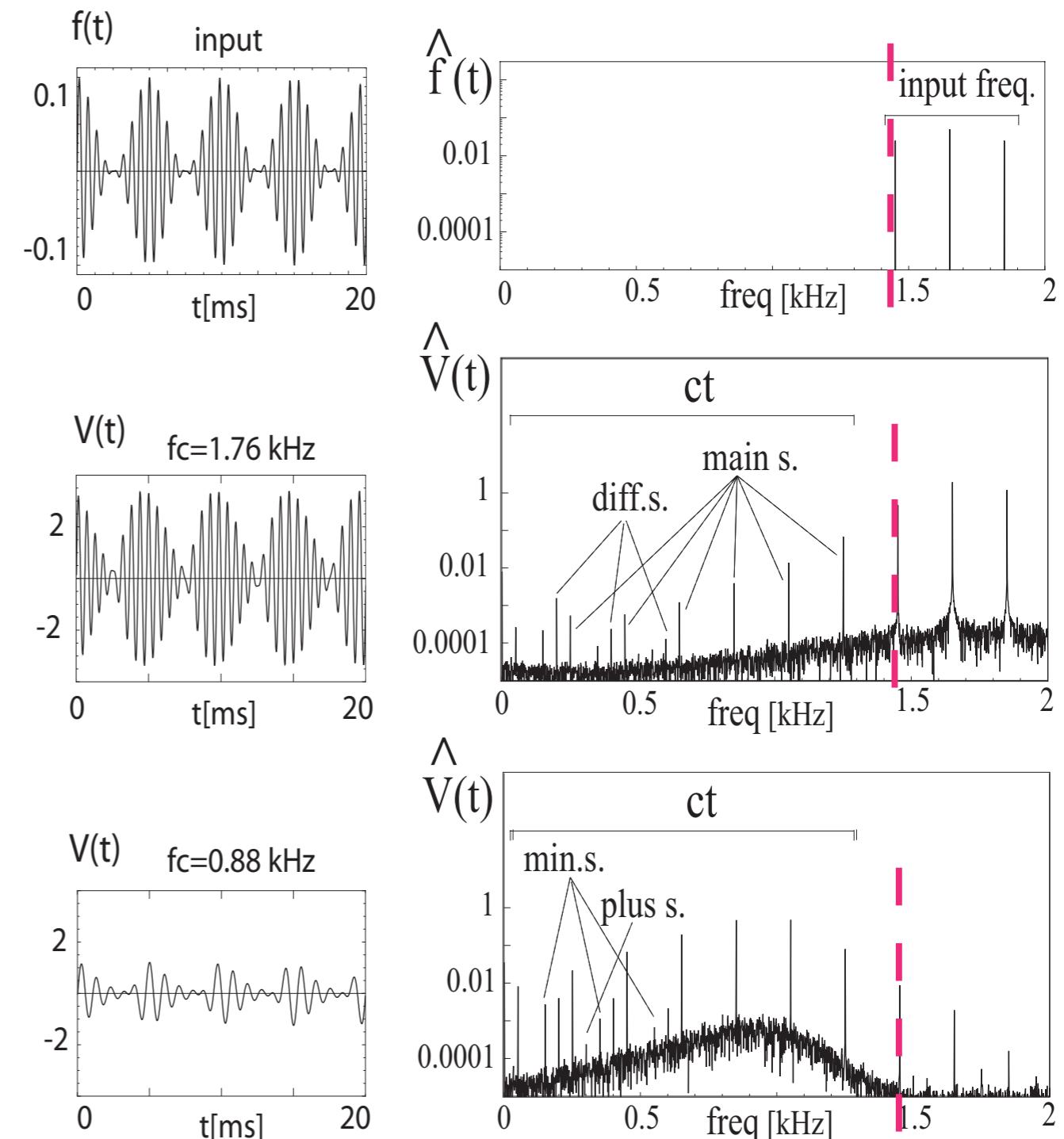
V Nonlinearity magic simple signals: complex networks!



inharmonic am tone $f(t)$, $A = 0.1$, $f_{car} = 1.65$ kHz,
 $f_{mod} = 0.2$ kHz; waveforms $f(t)$, $V(t)$, Fourier transforms



strong ct-generated signal at $f_c = 0.88$ kHz
 that classically should be absent!

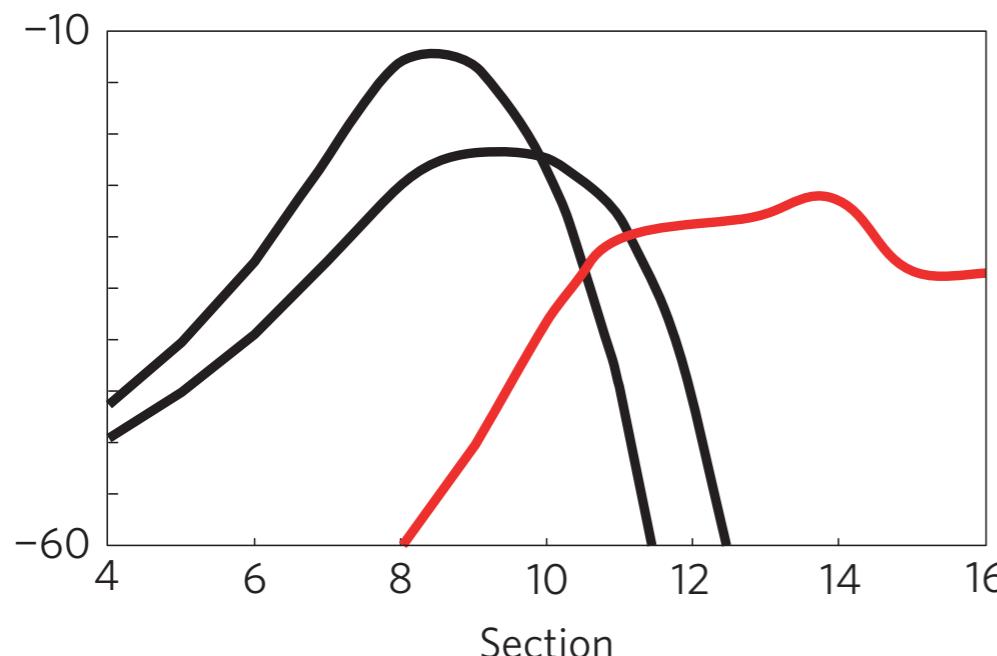


(pitch is physical: S.M. & R.S. PRL 2010)

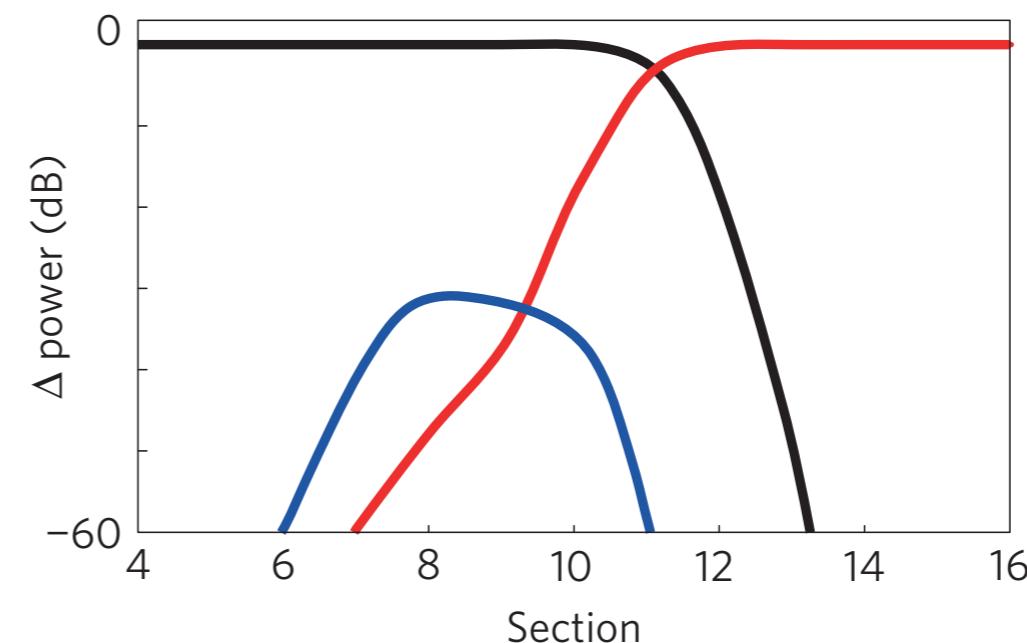
Combination tone saliency:

F.G. & R.S., Nat. Phys. 2014

Cochlear excitation for a complex two-tone stimulation (simulated) :



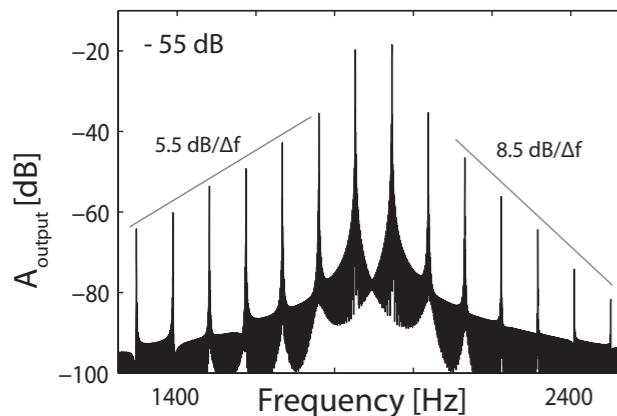
Black: signal power of frequencies f_2 and of f_1
Red: sum of lower CT ($f < f_1$)



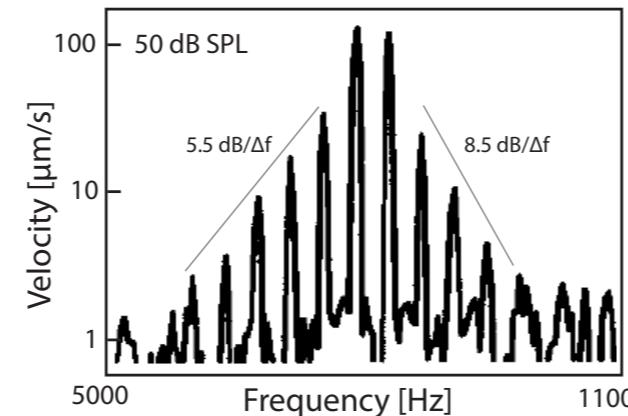
Black: added signal power from frequencies f_1 and f_2
Red: signal power of lower CT
Blue: signal power of higher CT ($f > f_2$) relative to total signal power.

Combination tones:

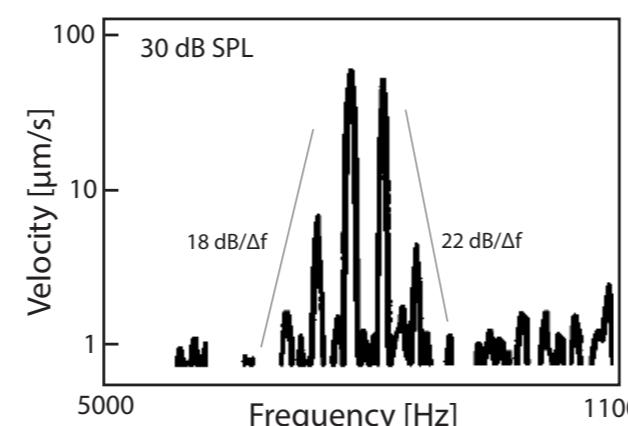
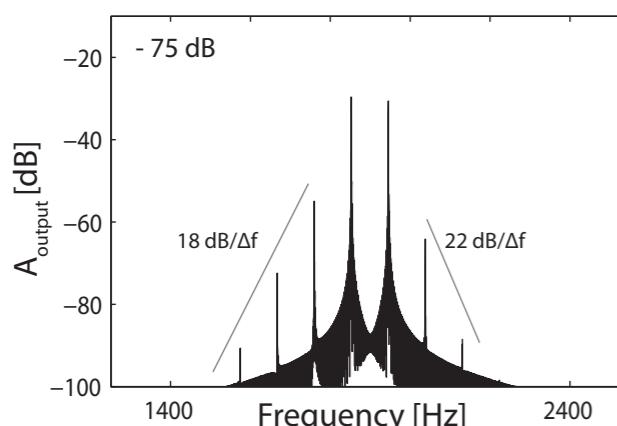
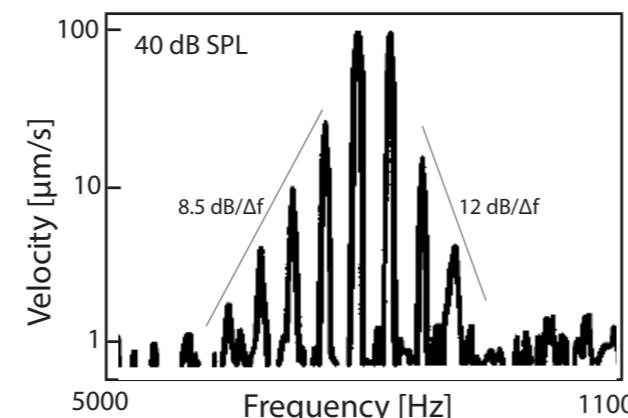
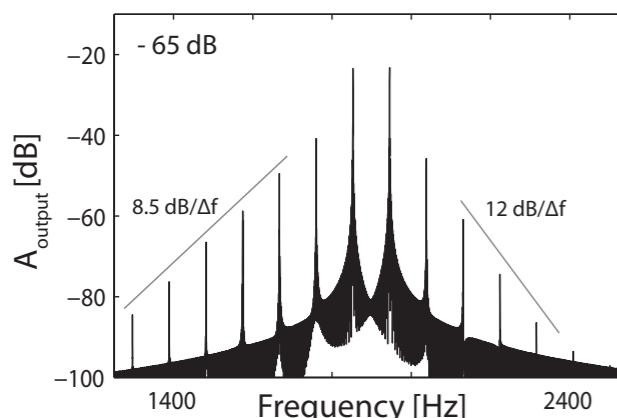
model



experiment

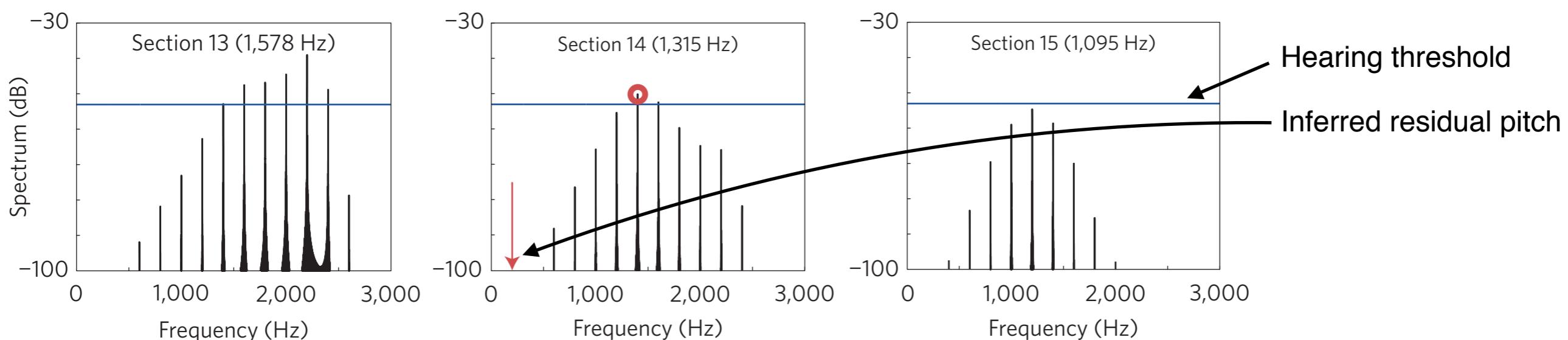
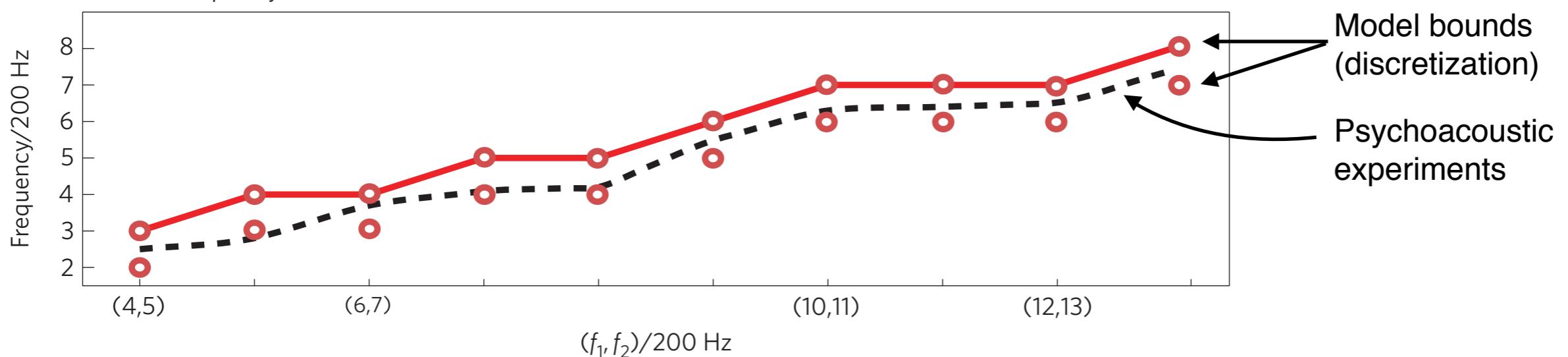


Place of measurement on the tonotopic map and choice of Hopf-cochlea section comparable (roughly one octave from cochlear base).



F.G. & R.S., Nat. Phys. 2014

Where is pitch read off ? Smoorenburg: Perceived pitch = Residual pitch at hearing threshold

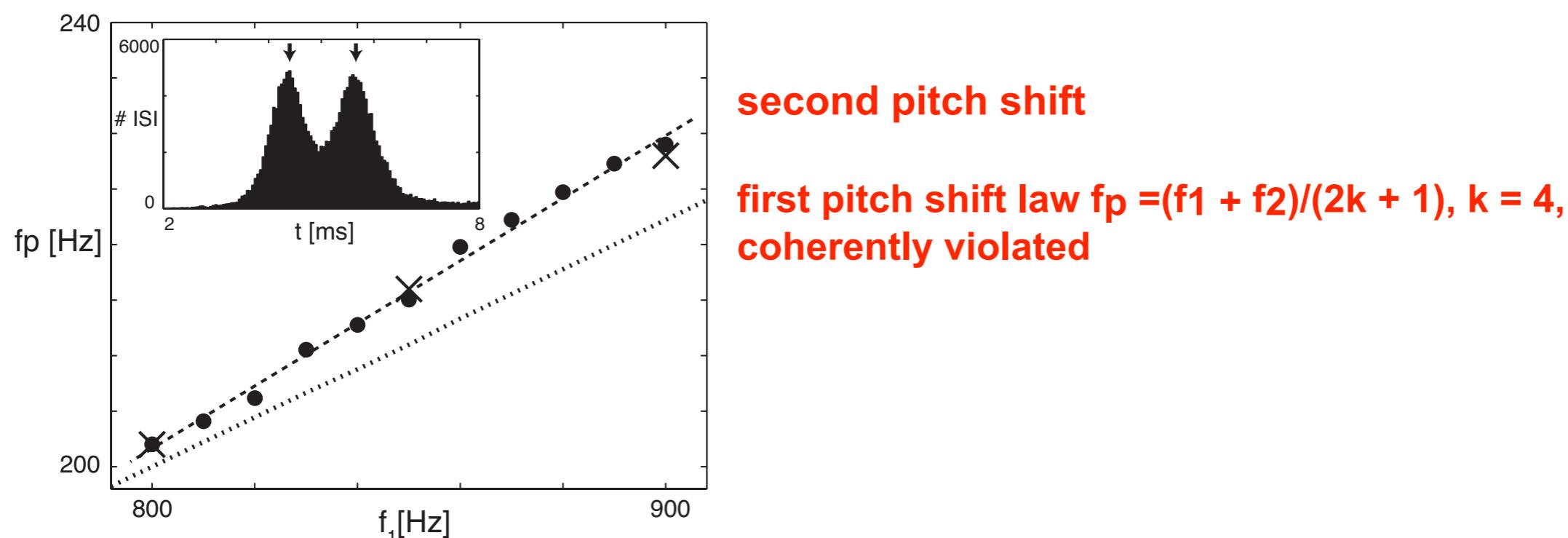
a**b**

F.G. & R.S., Nat. Phys. 2014

Second pitch shift effect

Two-frequency stimulation f_1 and $f_2 = f_1 + 200$ Hz, cochlea output at $f_c = 622$ Hz
(second pitch shift effect): psychoacoustic data (crosses), measured data (full dots)

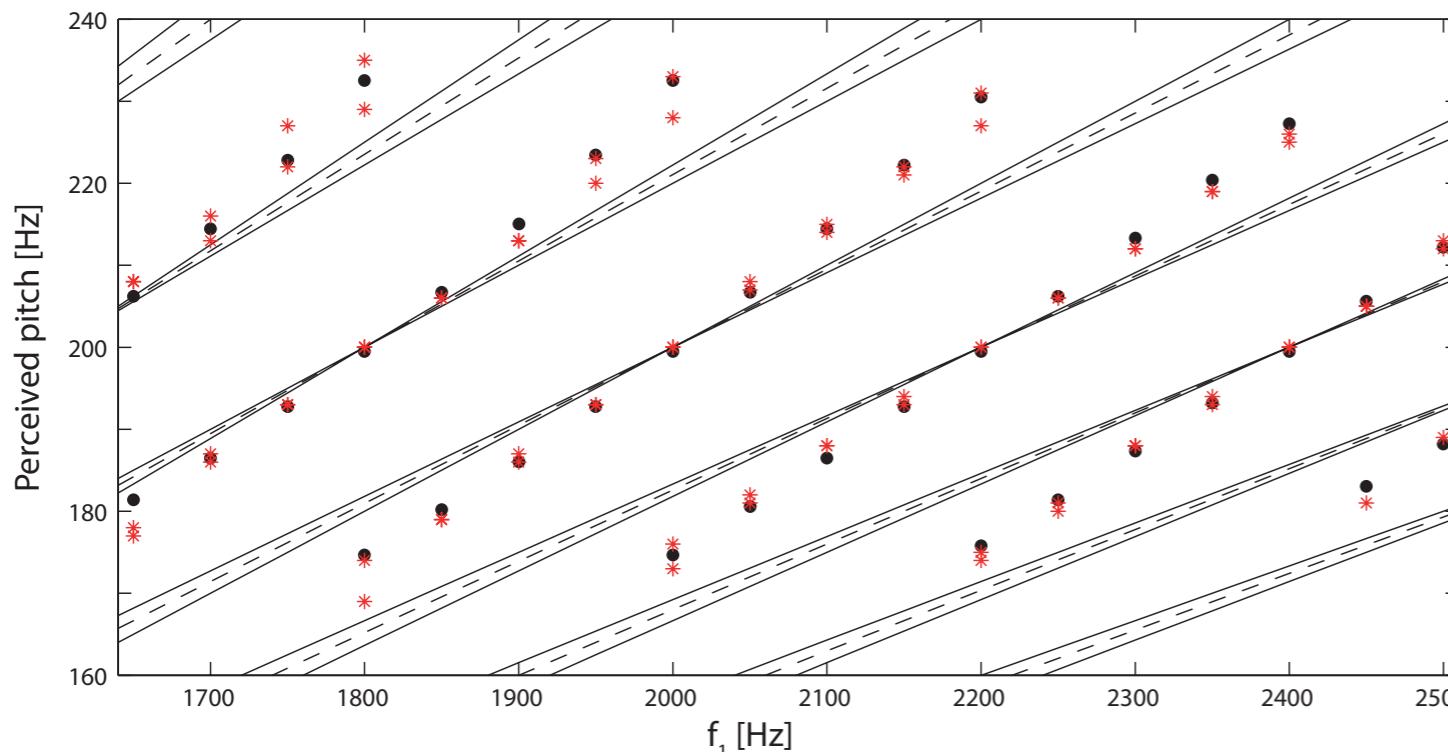
Inset: ISI-histogram for $f_1 = 900$ Hz, showing fp for $k = 4$ (left peak, for the rightmost cross) and for $k = 5$ (right peak, cross at $fp < 178$ Hz)



Inset: ISI-histogram end of auditory nerve (S.M., F.G. & R.S. Sci. Rep. 2015)

Second pitch shift:

red: psychophysical experiments; black: model



Two-frequency stimuli with $f_2 = f_1 + 200$ Hz.

Red: Psychoacoustic data (partial amplitudes 40 dB SPL)

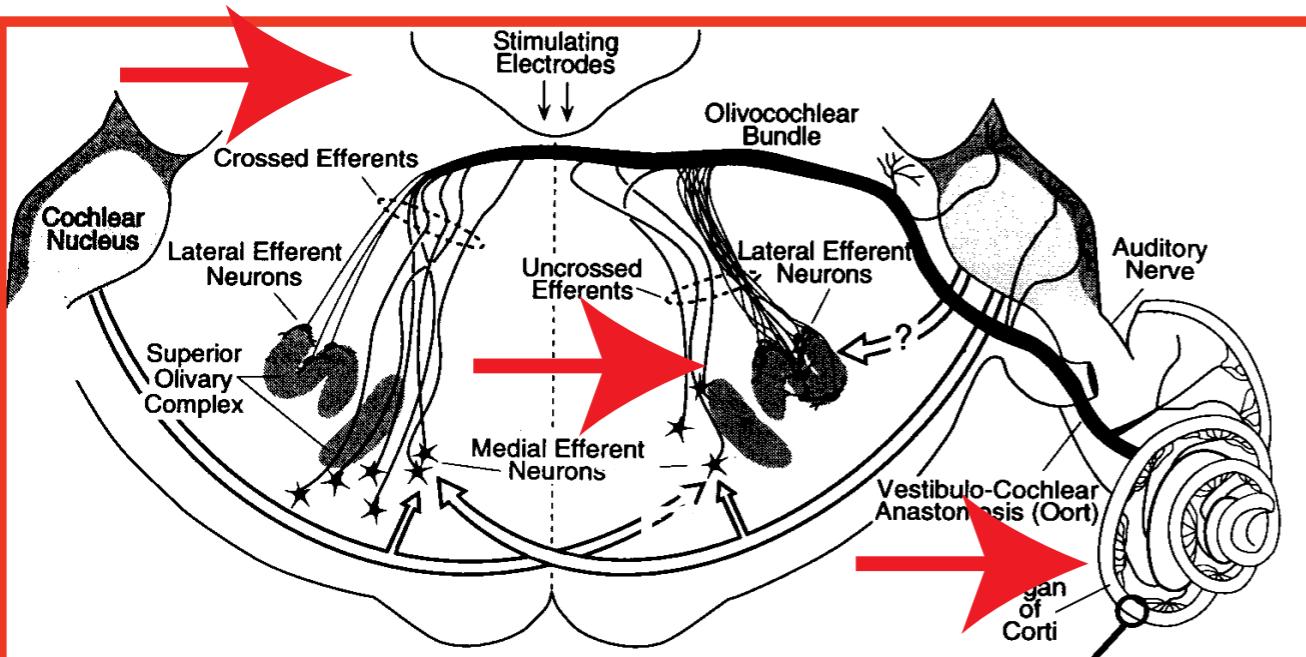
Black: Hopf cochlea simulation (7th section with $f_{ch} = 1245$ Hz, partial amplitudes -63 dB).

Solid lines: classical predictions of the perceived pitch.

: solves Ohm-Seebeck dispute !

second pitch shift due to cochlear fluid: F.G. & R.S. Nat. Phys. 2014,
requested slight ‘tuning’ of the Hopf amplifiers (no-flat tuning of Hopf parameters)

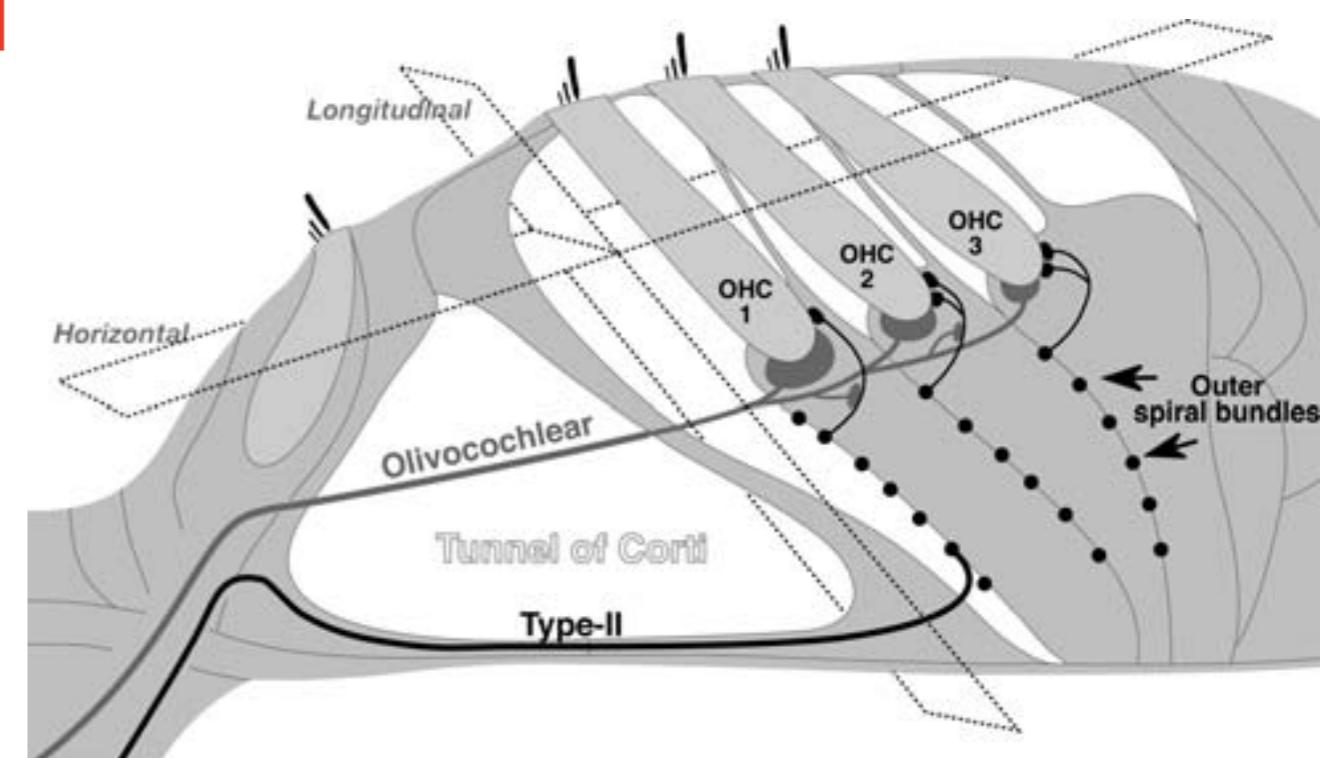
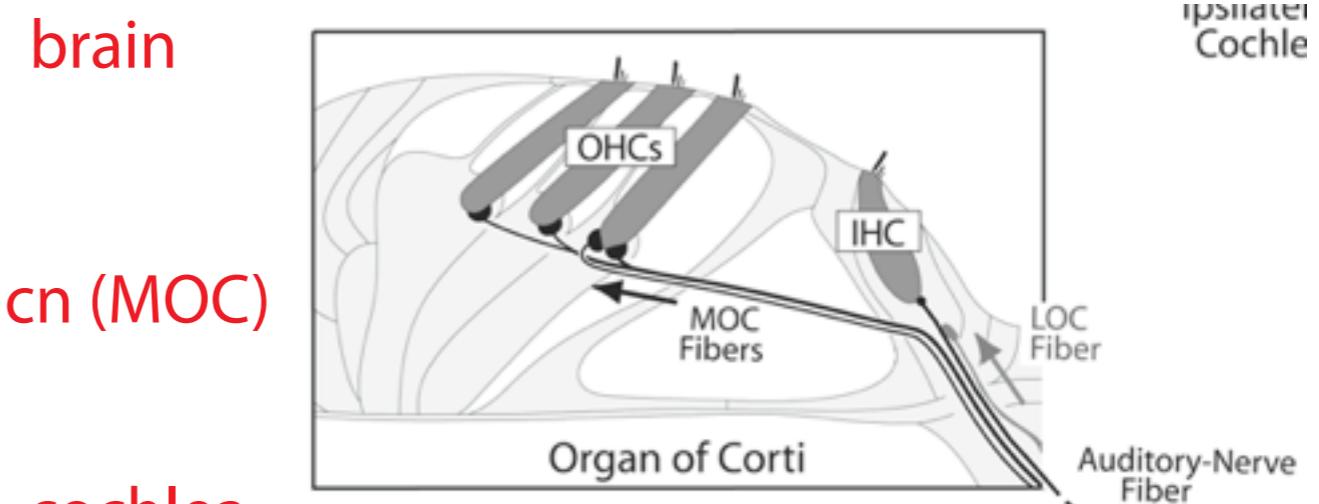
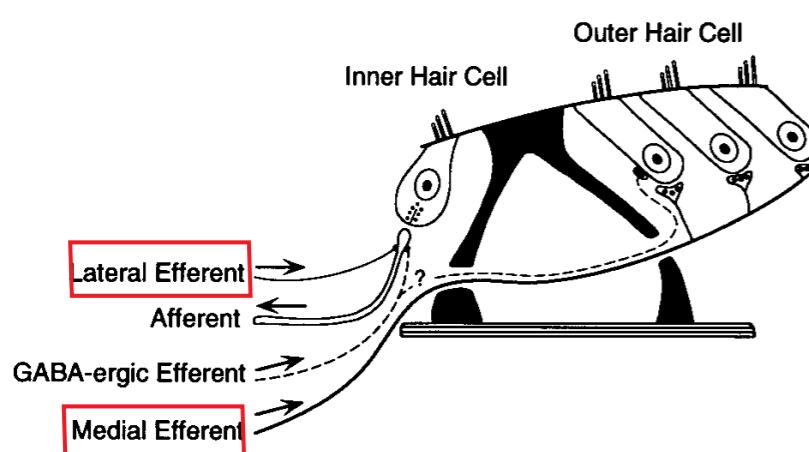
Anatomical embedding



brain

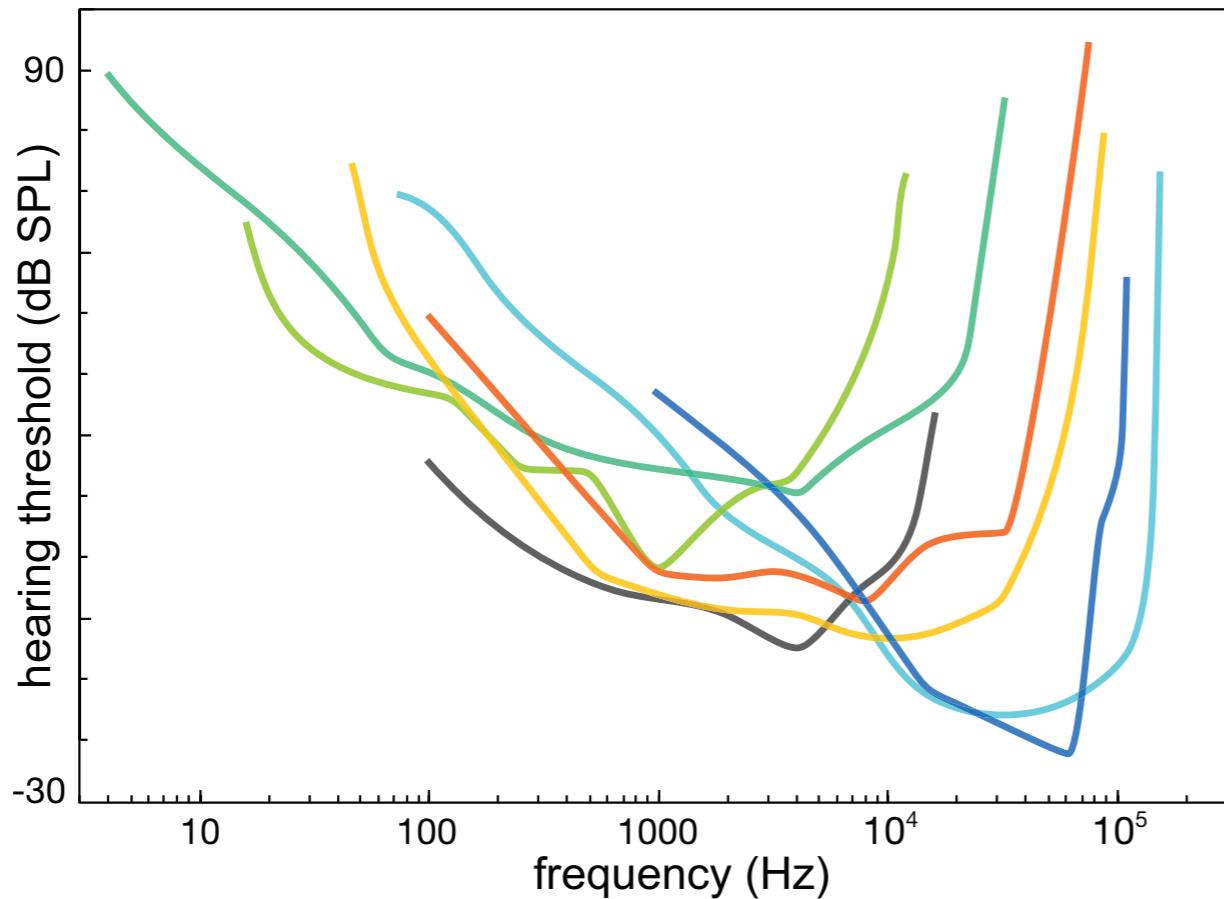
cn (MOC)

cochlea



VI Hearing threshold

Animal evidence (nonspecialists)

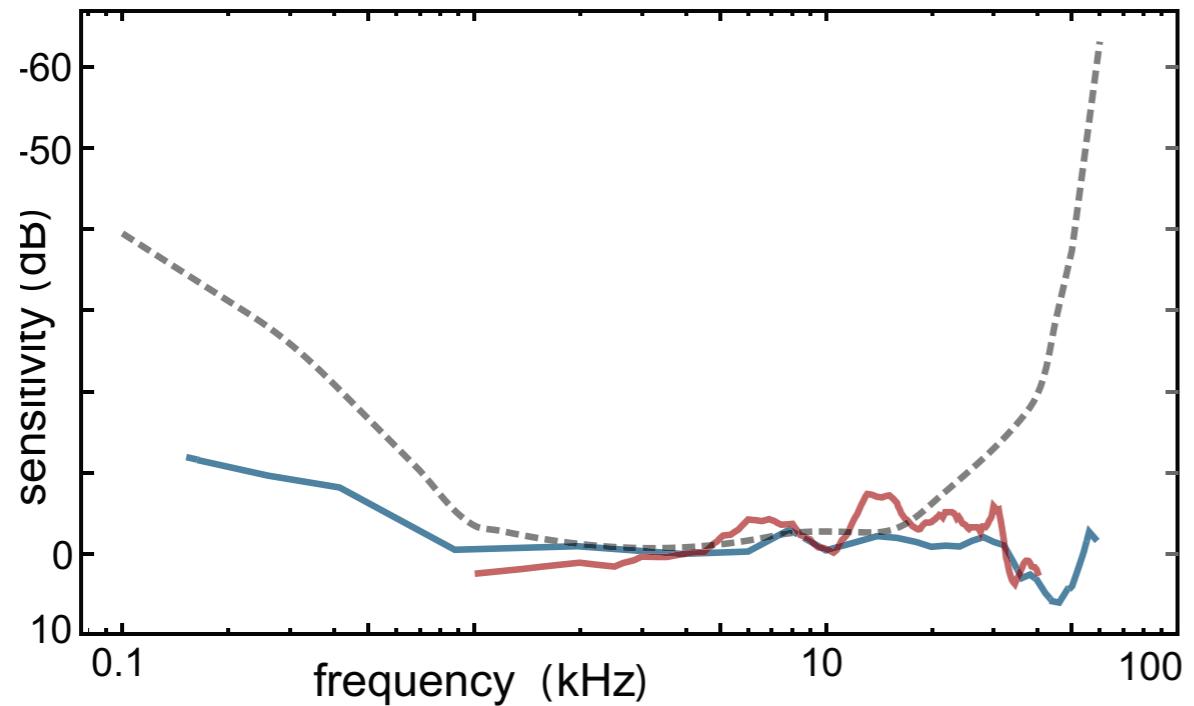


Dogma : Frequency dependence of the hearing threshold is exclusively determined by outer and middle ear

Behavioral audiograms (from top to bottom):

Prairie dog [23], elephant [24], lemur [25], domestic cat [26],
human psychoacoustical hearing threshold [4],
white-beaked dolphin [27], false killer whale [28].

Animal evidence



Ruggero and Temchin 2002

Outer-middle ear transfer functions Mongolian gerbil

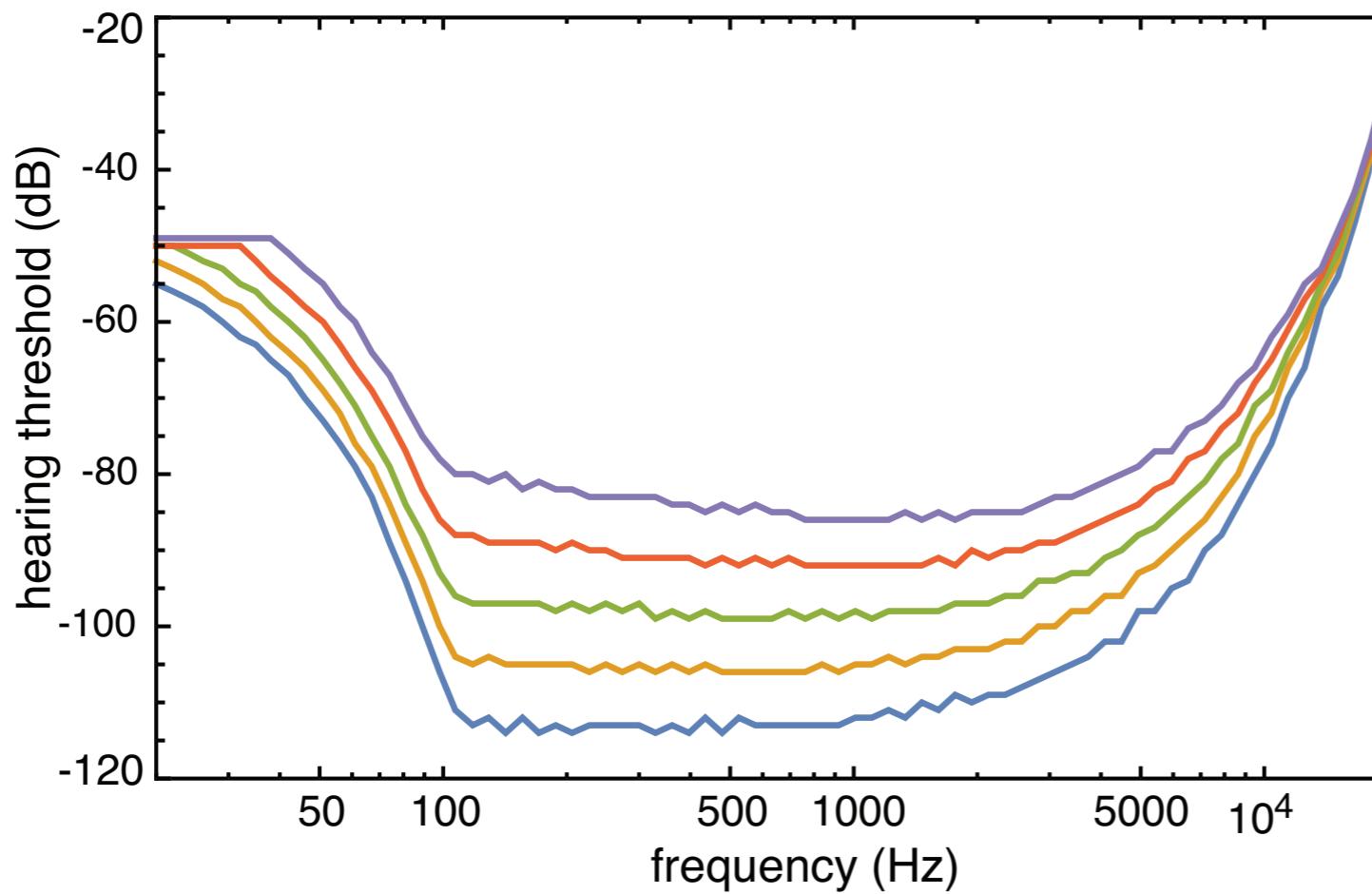
Dashed: Behavioral hearing threshold

Blue: Pressure in scala vestibuli near stapes footplate

Red: Stapes velocity

Could it be the cochlea?

flat-tuned cochlea:



flat tunings: $\mu^{(j)} = \text{constant}$

Hopf cochlea with $N=29$ sections
 $f_{ch} = 110 \dots 14080$ Hz

$\mu^{(j)}$ is the same for all sections:

$\mu^{(j)} = -0.40$

$\mu^{(j)} = -0.35$

$\mu^{(j)} = -0.30$

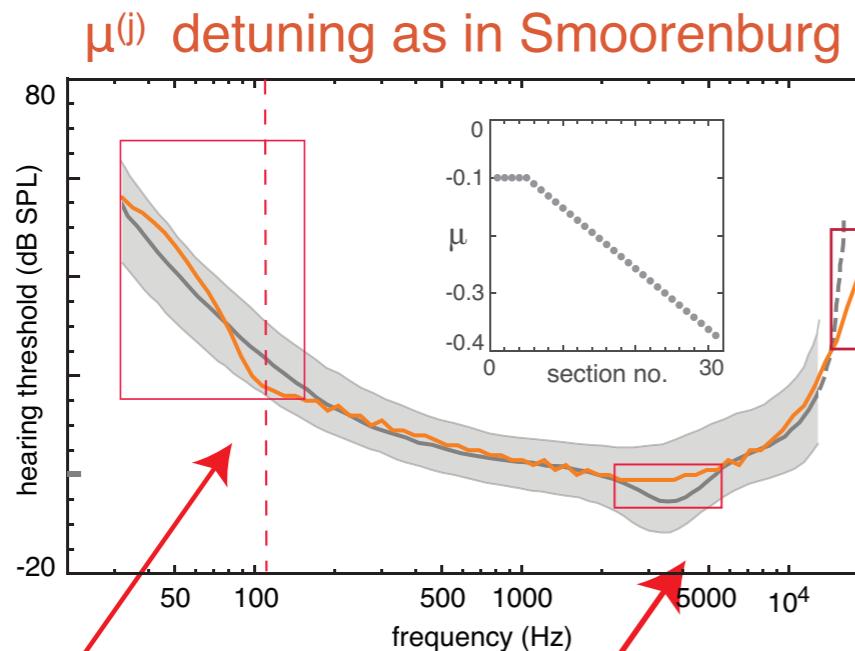
$\mu^{(j)} = -0.25$

$\mu^{(j)} = -0.20$

F.G., K.K., T.L. & R.S. submitted

1. Response of section j is defined as $R_j = 20 \log_{10}[\max(\text{Re}(\text{out}_j))]$
2. The maximal response of Hopf cochlea is $R_{\max} = \max(\{R_j : j = 1, 2, \dots, N\})$
3. Hearing threshold of a pure tone stimulus $F(t) = A \exp(-i2\pi ft)$: defined as the input level $L = 20 \log_{10}[A]$ that gives rise to $R_{\max} \approx -50$ dB
4. 0 dB SPL input in experiments corresponds to -114 dB input to Hopf cochlea

Tuning of amplifiers



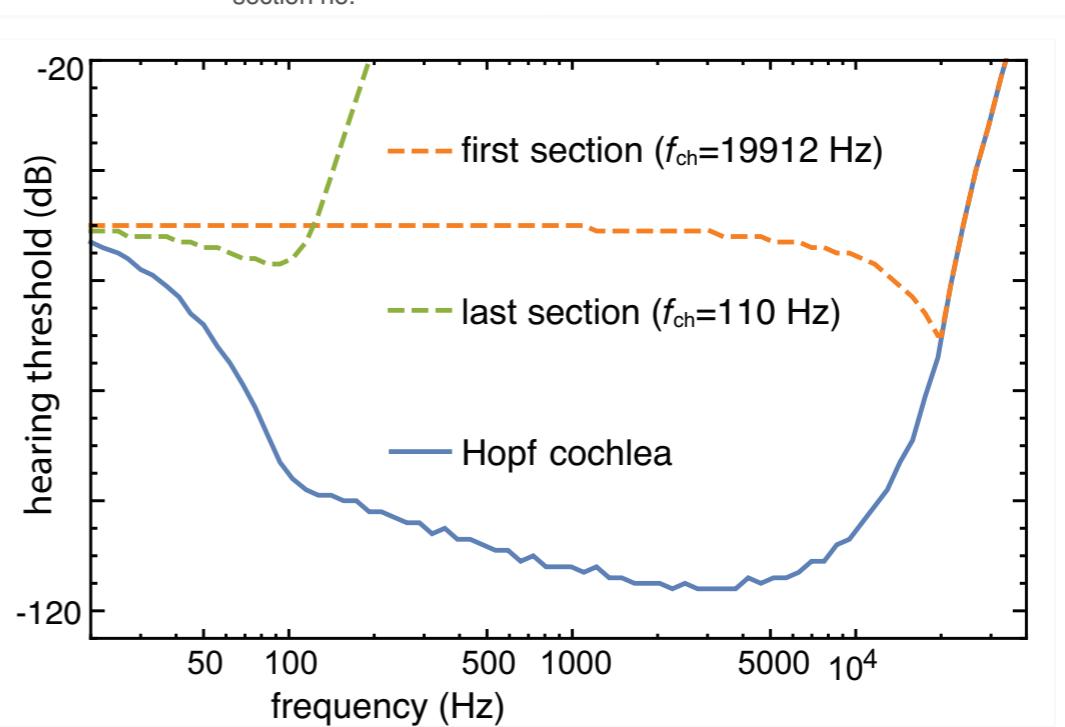
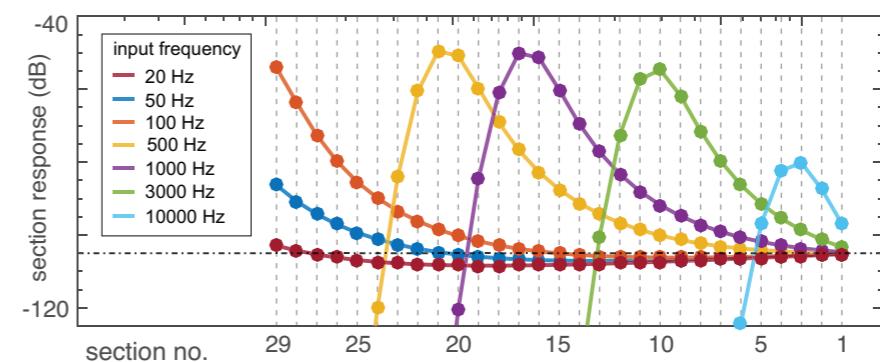
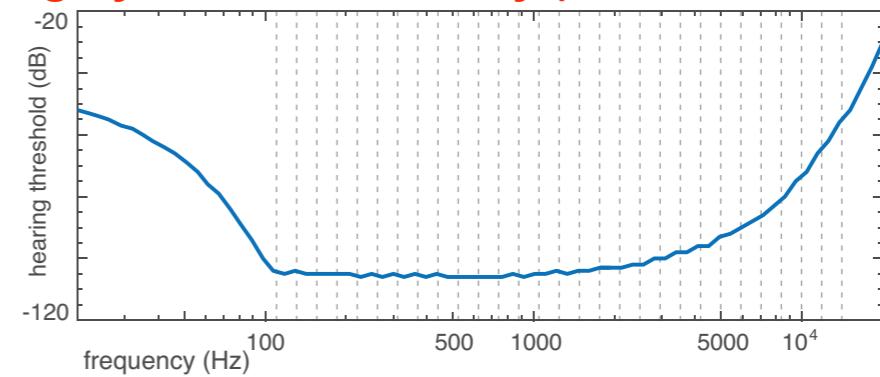
discretization effect

resonance middle/outer ear: <10 dB,
around 4000 Hz (Shaw 1974):
Perfect agreement

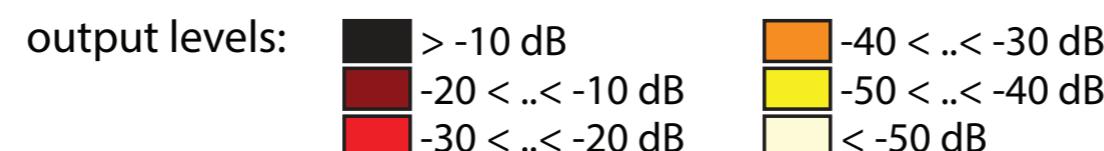
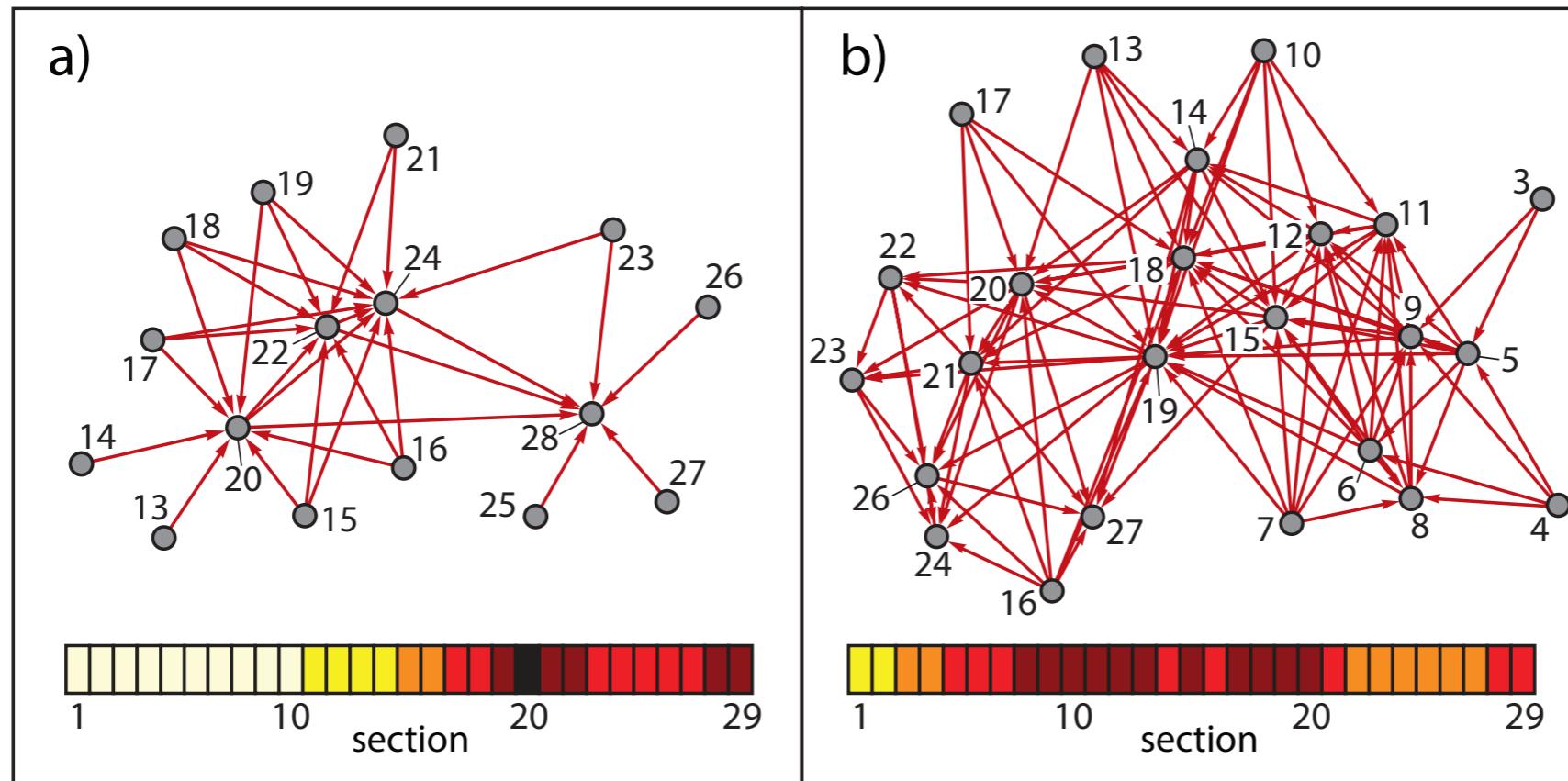
contradiction to schoolbook
wisdom ..

no data available

gray: human variability (Fastl / Zwicker 2007)



VII Activation networks are the signal..



a) two pure tones input (3/8, 1/2 kHz)

b) two complex tones (2, 3.35 kHz, with 5 harmonics each)

Cochlea: 29 sections, covering (0.11, 14.08) kHz on a logarithmical scale; $\mu=-0.25$ at all sections; input: -60 dB each tone.
Upper: Activated networks ('above hearing threshold'), lower: corresponding activations on the unrolled cochlea.

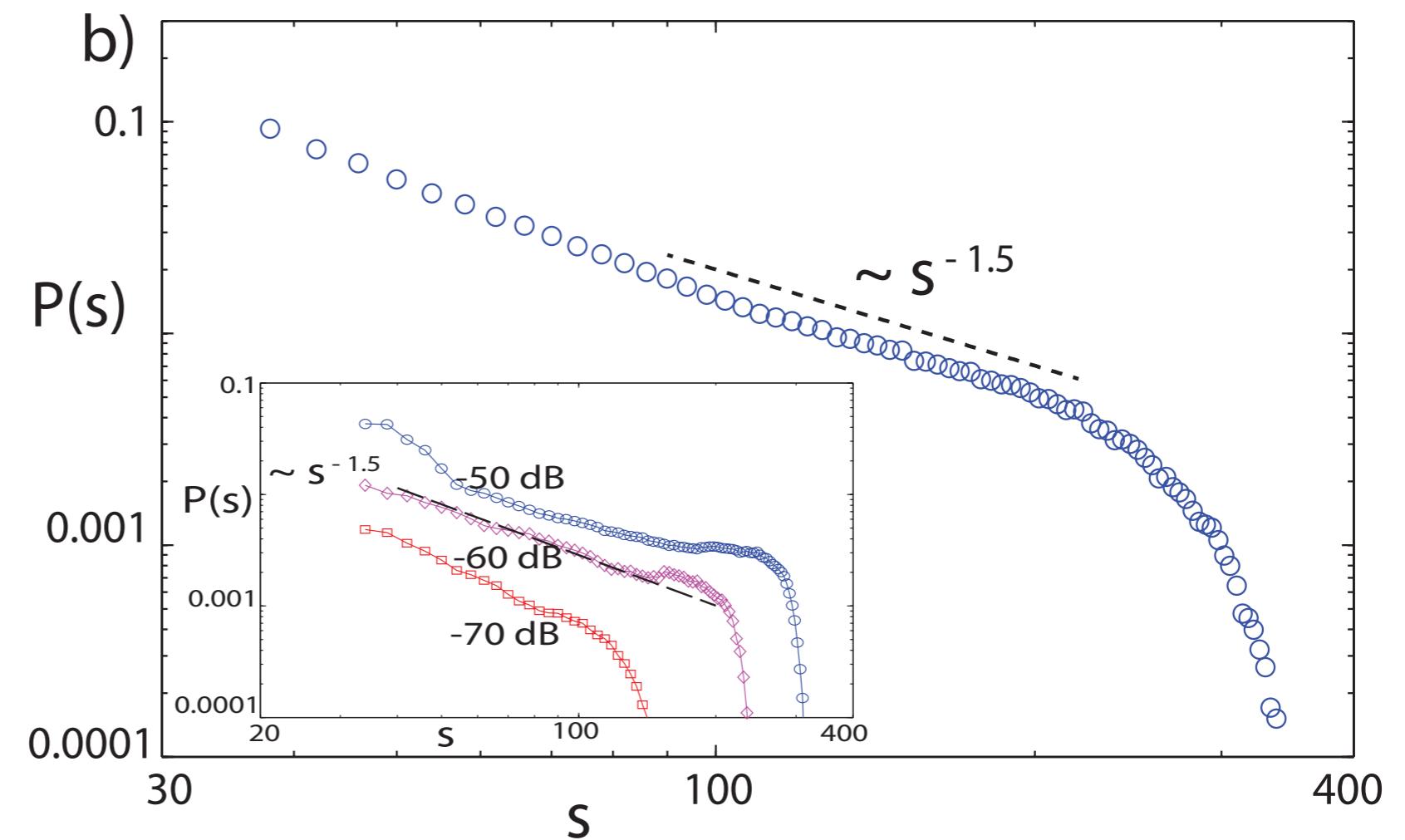
(R.S. & F.G. PRL 2016)

VIII Hearing @ criticality?

Two complex tones (random amplitude and frequency): **s: size of activation network by number of links**

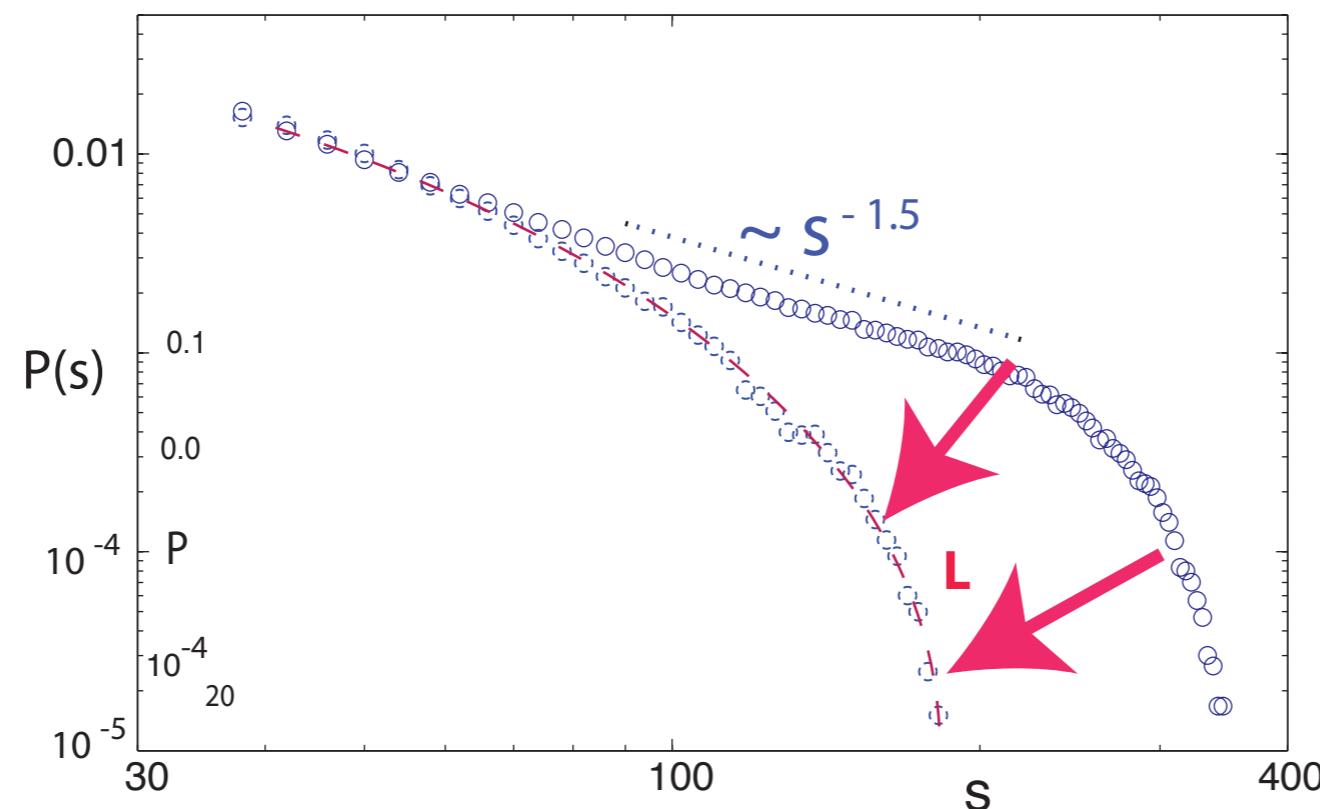
Inset: fixed amplitudes:
subcritical, critical, supercritical

power-law activation networks!



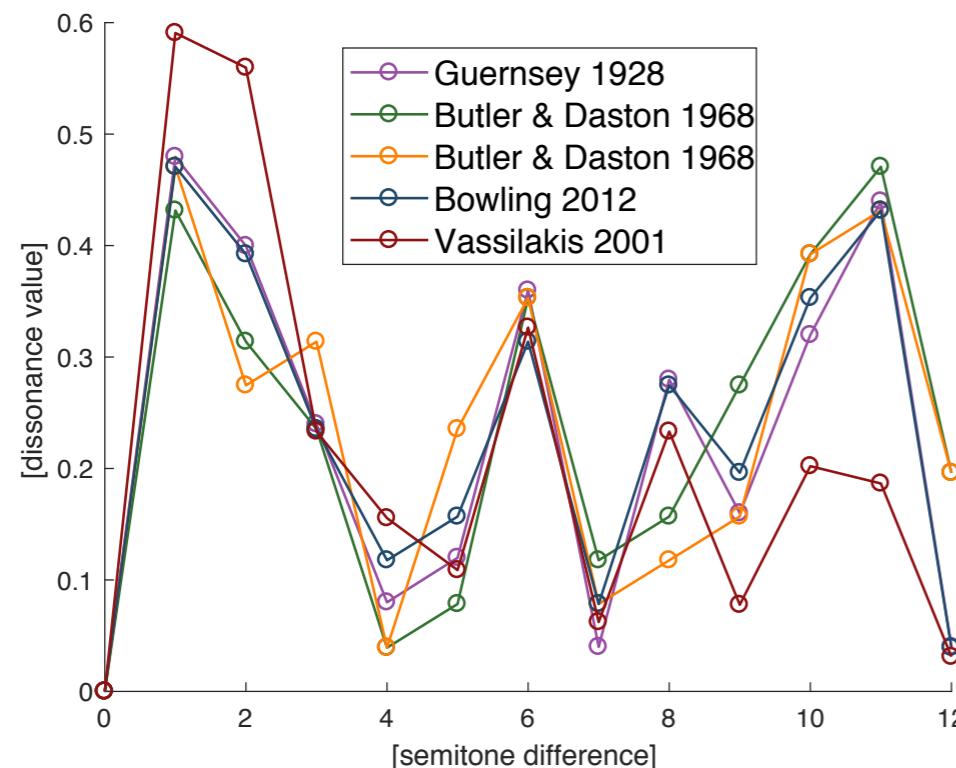
(R.S. & F.G. PRL 2016)

Statistical meaning of learning



Detuning of two frequency bands (nodes 15,16 and nodes 19,20,21) from $\mu = -0.25$ to $\mu = -2.0$:
The initial power-law distribution $s^{-1.5}$ changes into a strictly convex distribution shape (line L)!

IX When is a sound perceived harmonic?



Dissonance vs. interval length:
Not cultural, but strong experimental variations

Short history of consonance and dissonance:

Pythagoras (6th century BC):

Strings of simple length ratios elicit sensations of pleasantness (“consonance”).

Intervals of the octave (2:1), the perfect fifth (3:2) and the perfect fourth (4:3) provide the Pythagorean tuning.

Geoseffo Zarlino (renaissance music theorist):

Added the intervals of the major third (5:4), minor third (6:5) and major sixth (5:3) to the consonance set.

Daniel Bernoulli: Superposition of infinite harmonic vibrations on a vibrating string;

Marin Mersenne, Leonhard Euler and Joseph Fourier: Concept of a “harmonic series”.

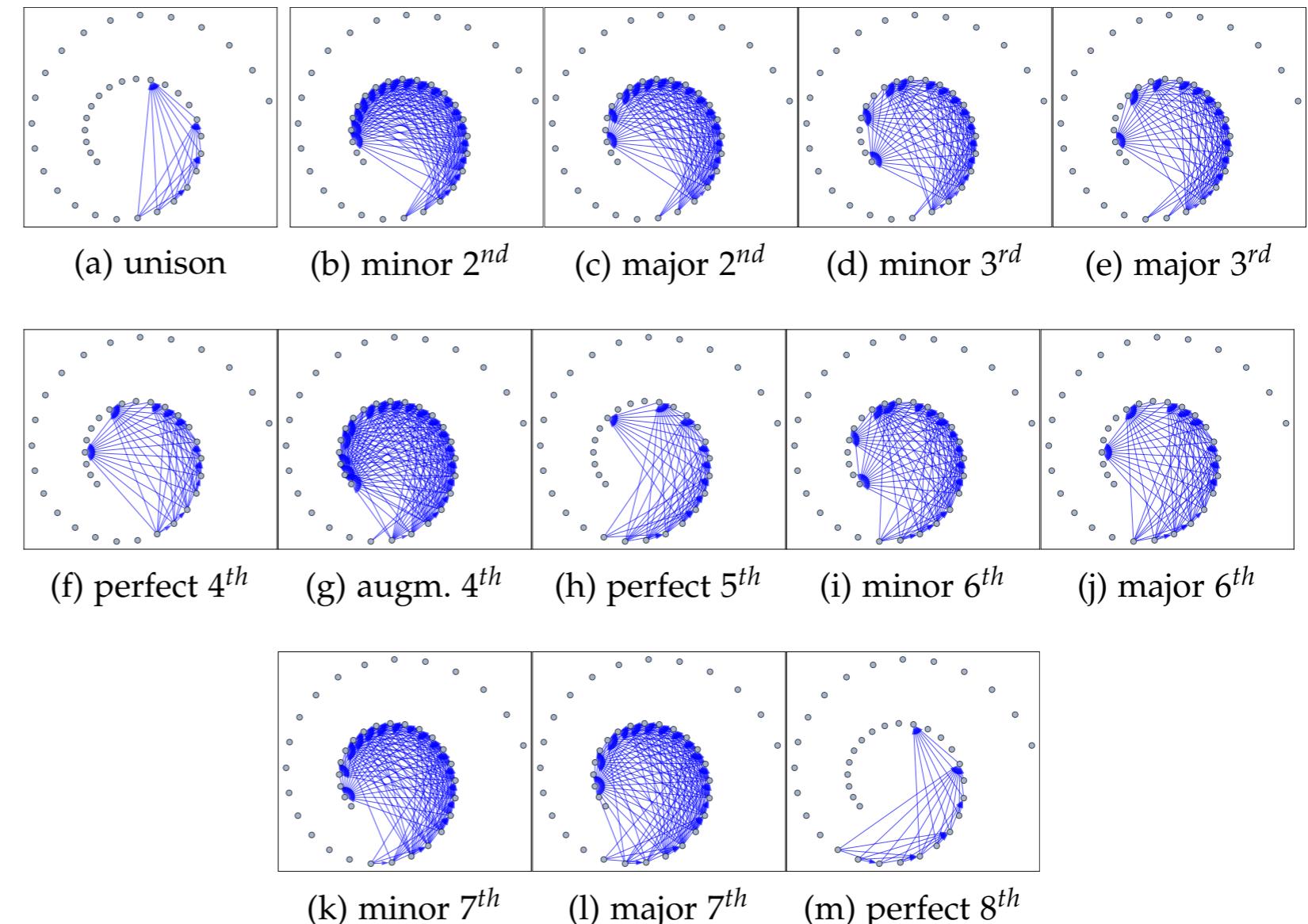
Professionals vs. amateurs: Identically perceived

Network property?

Pure tones vs, complex tones: Distinctly perceived

Network picture

Higher dissonance \longleftrightarrow
larger activated network size,
larger edge density



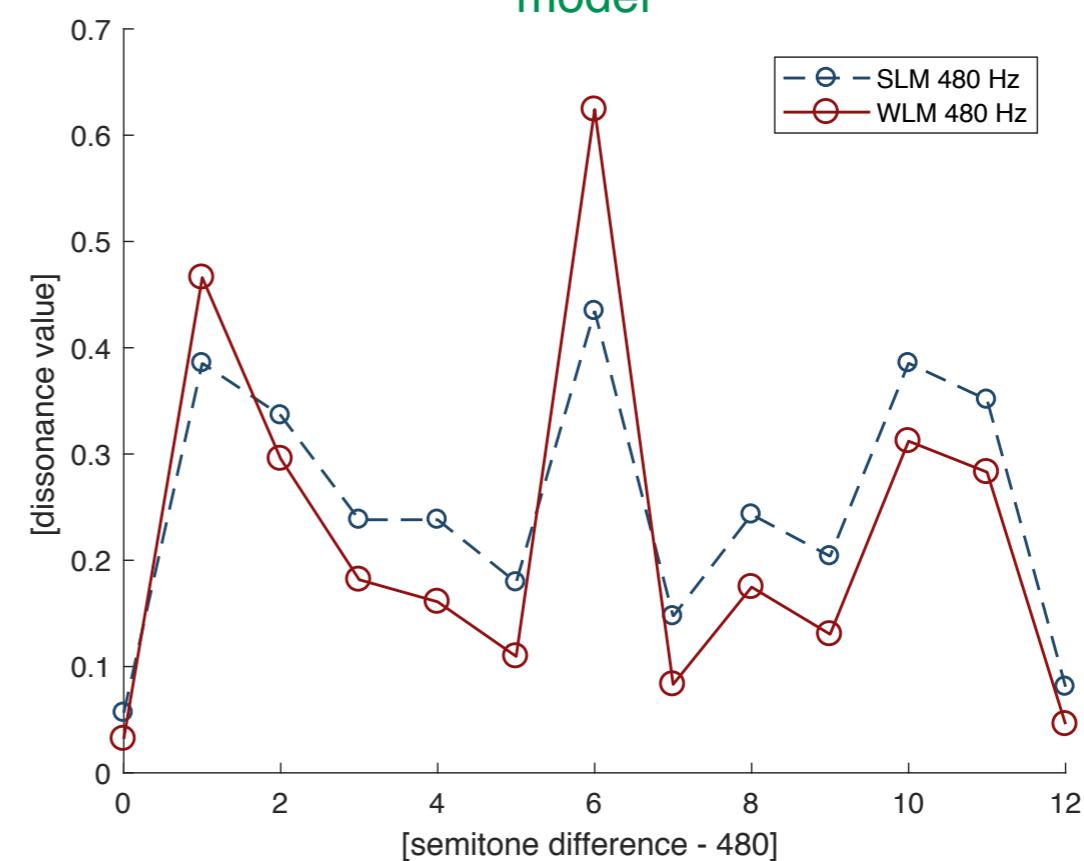
Network-based measures of dissonance:

- Topological graph: Network size of active nodes (SLM)
- Weighted graph (WLM)

Network measure vs. psychoacoustics:

experiment

model



Not perfect, but a good match!

Perspectives of this approach:

- **perfect restitution of human hearing**
- **new generations of technical sound sensors**
- **dealing efficiently and coping with ‘big data’**

Fundamental human perception ‘reduced’ to cochlear physics and network theory

**: Physics / engineering approach
brings us closer towards the “human mind”**

thanks for listening..

Measuring listening efficacy

(F.G, V.S., N.B., R.S., Phys. Rev. Appl. 2014)

models of pitch perception suggest comparison:

- SACF: sum of normalized autocorrelations of each section's output
vs.
- NACF: normalized autocorrelation of the target signal desired signal x / unwanted signal y / f_i output of i -th section

$$TE(x, y) := \frac{\|\text{NACF}(x) - \sum_i \text{NACF}(f_i(x + y))/N\|_2}{\|\text{NACF}(y) - \sum_i \text{NACF}(f_i(x + y))/N\|_2}$$

→ TE in $[0, \infty]$:
high ($>>1$) TE: bad tuning, low (<1): (very) good tuning
:TE-optimization problem in multidimensional μ -space

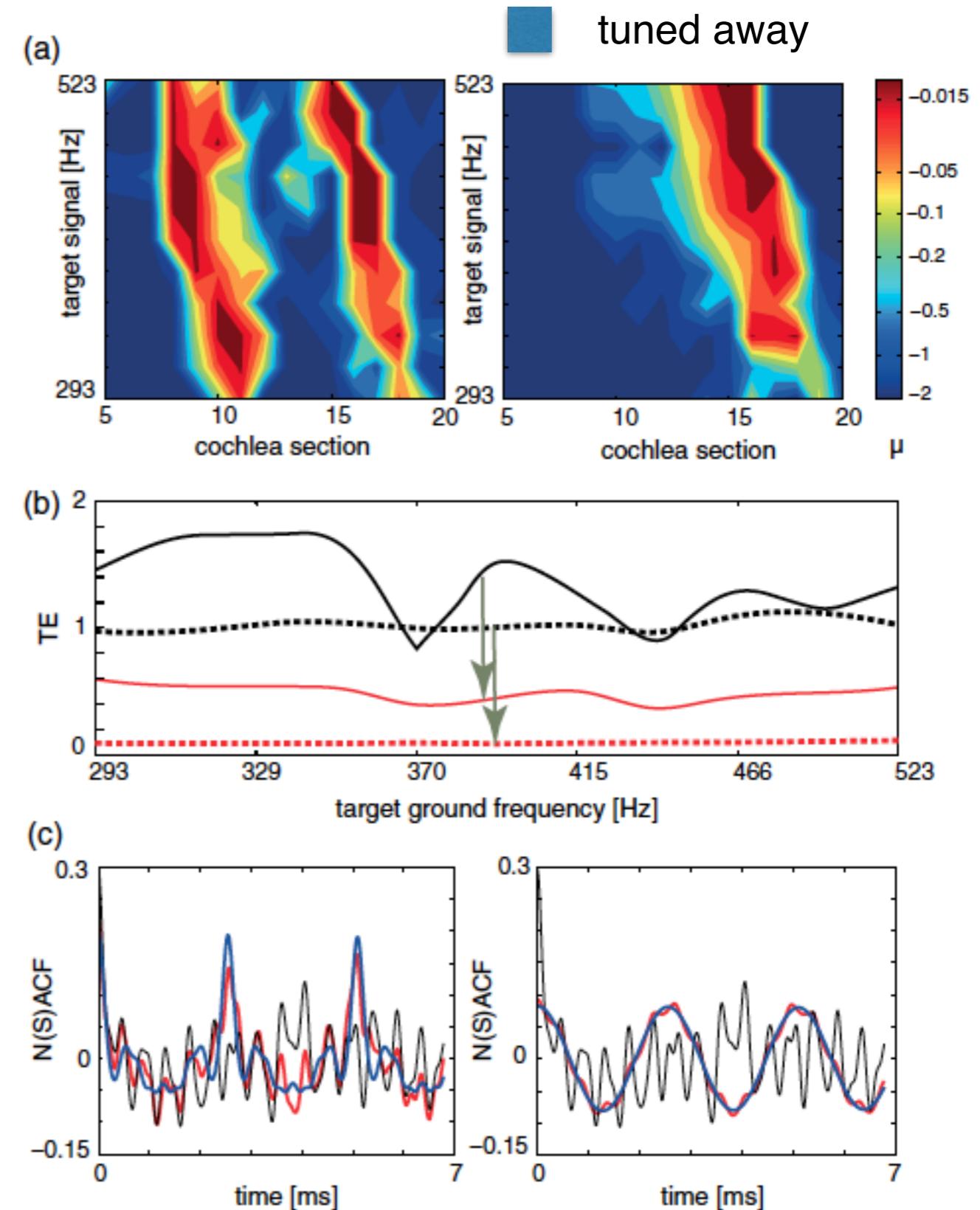
Results :

two complex instruments:
'Flute' vs.'Zinke'(both parts of church organs)

Tuning patterns: red: close to bifurcation,
blue: away from bifurcation.
red: close to bifurcation,

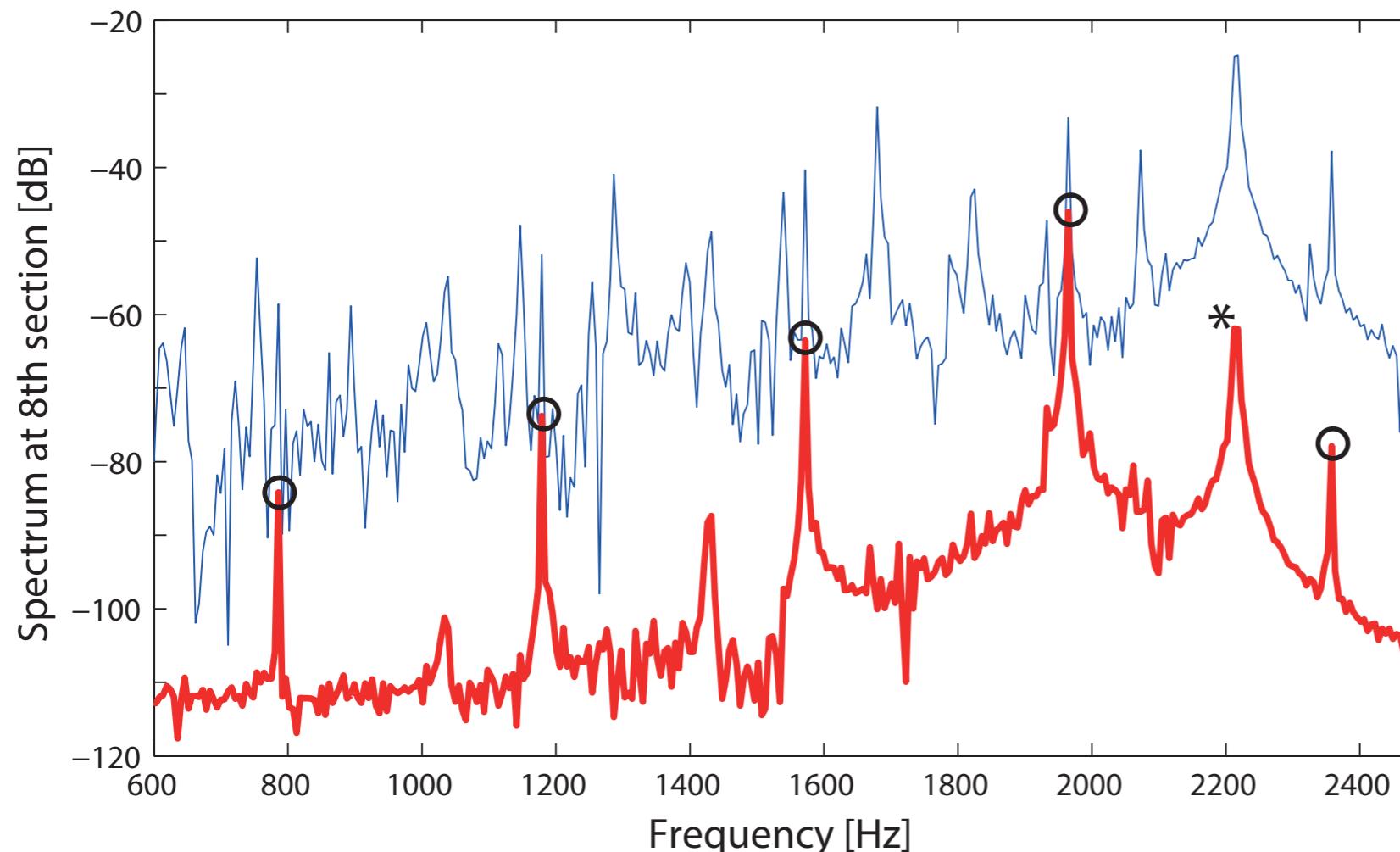
a) left: sweeping "Reel" target
right: sweeping "Flute" target
(tuning towards "Reel" requests
enhancement of the 3rd and 5th harmonics
(two parallel reddish stripes)

TE consistently < 1:
strong target enhancement
Black: flat tuning; red: TE-tuning



(F.G, V.S., N.B., R.S., Phys. Rev. Appl. 2014)

Using pitch as guiding control feature:



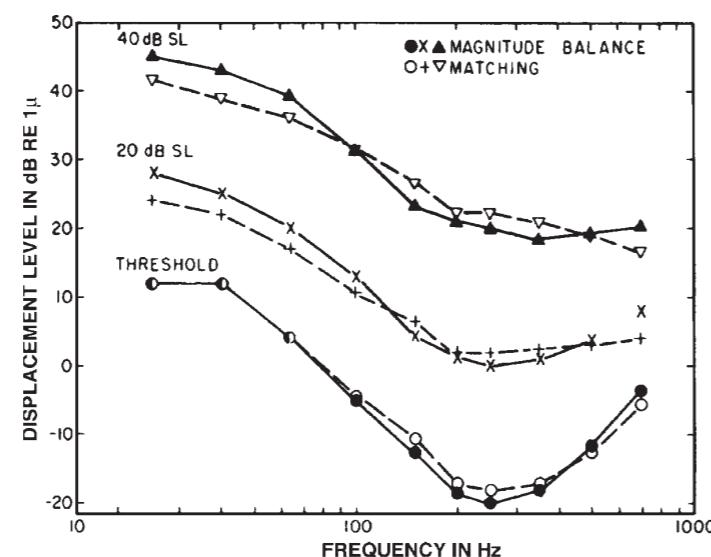
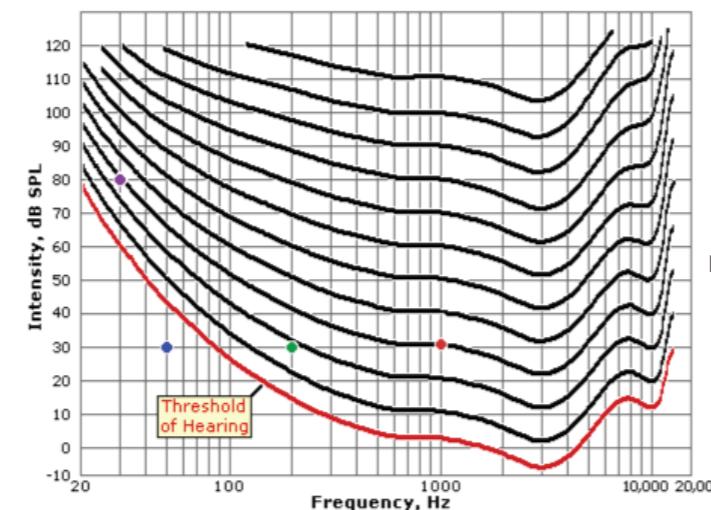
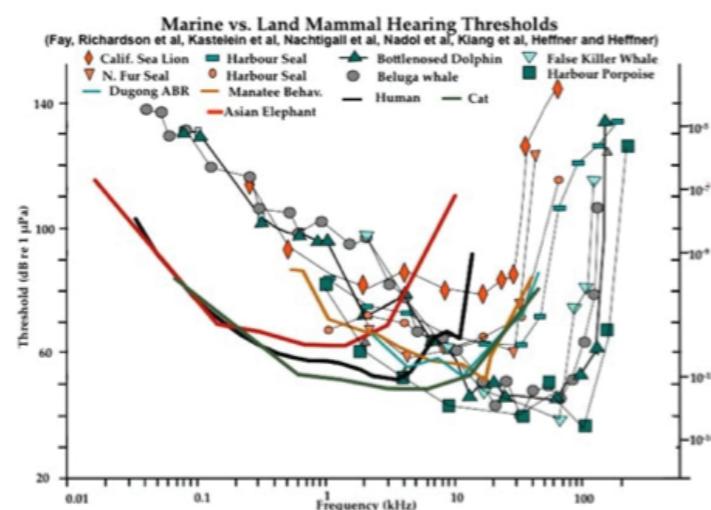
original: flute and reel

disturber (flute) and
crossproducts removed;
harmonic series restored

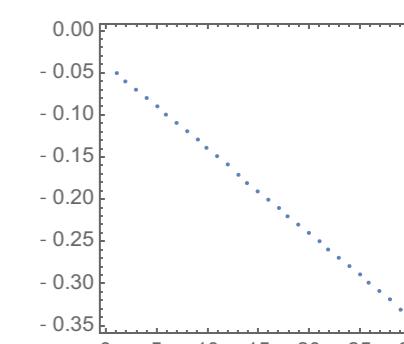
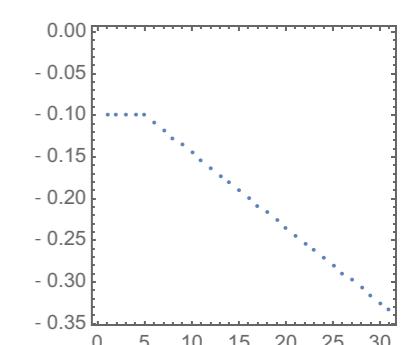
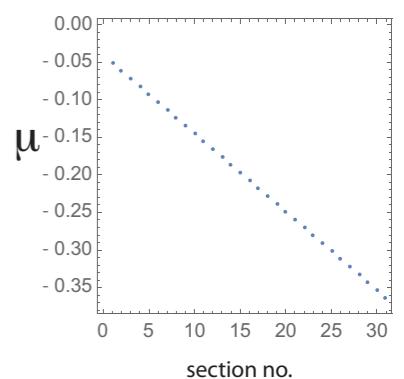
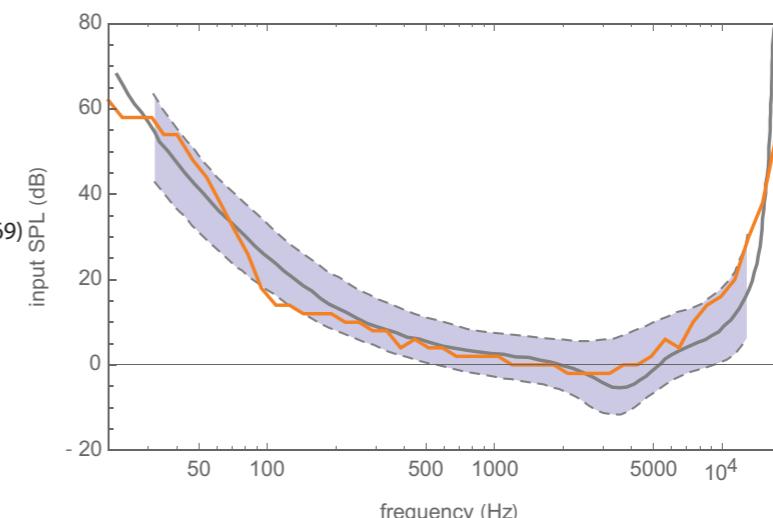
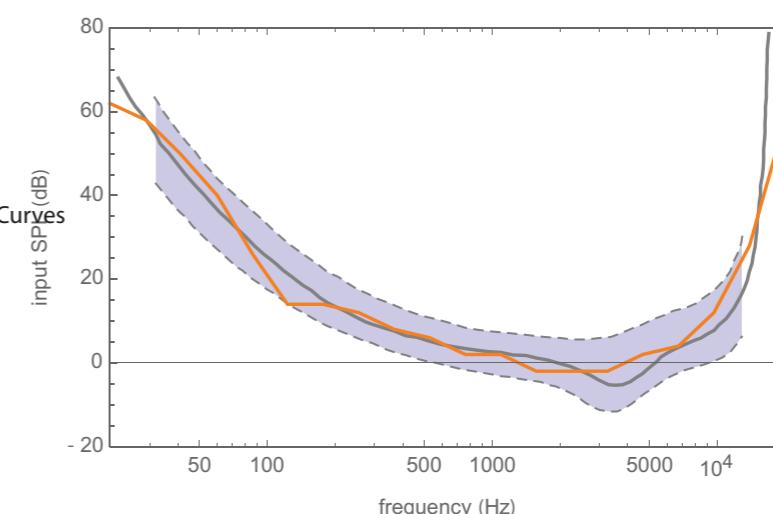
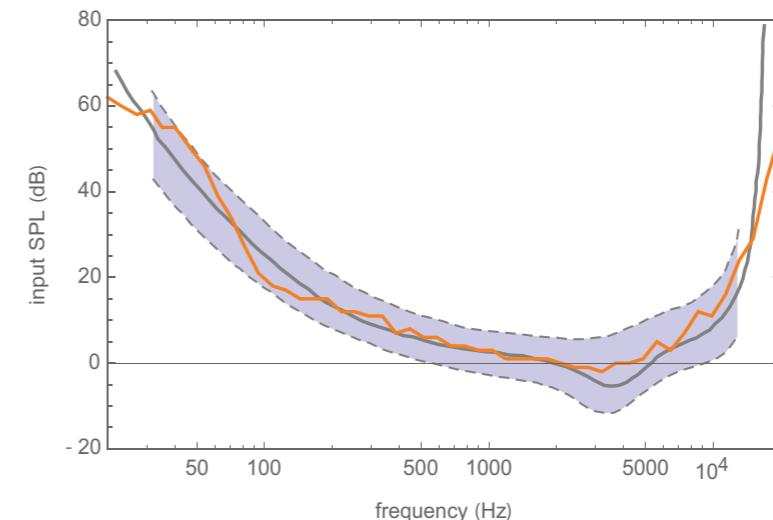
: efficient biomorphic tool for source separation!

(F.G.,V.S.,N.B., R.S.. Phys. Rev. Appl. 2014)

Hearing threshold



Verrillo, R.T., Fraioli, A., and Smith, R.L. Sensory magnitude of vibrotactile stimuli. *Percept. Psychophys.* 6: 366–372, 1969..



Measuring listening efficacy

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