

Present status of a superconducting rotating gantry for carbon therapy



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Outline

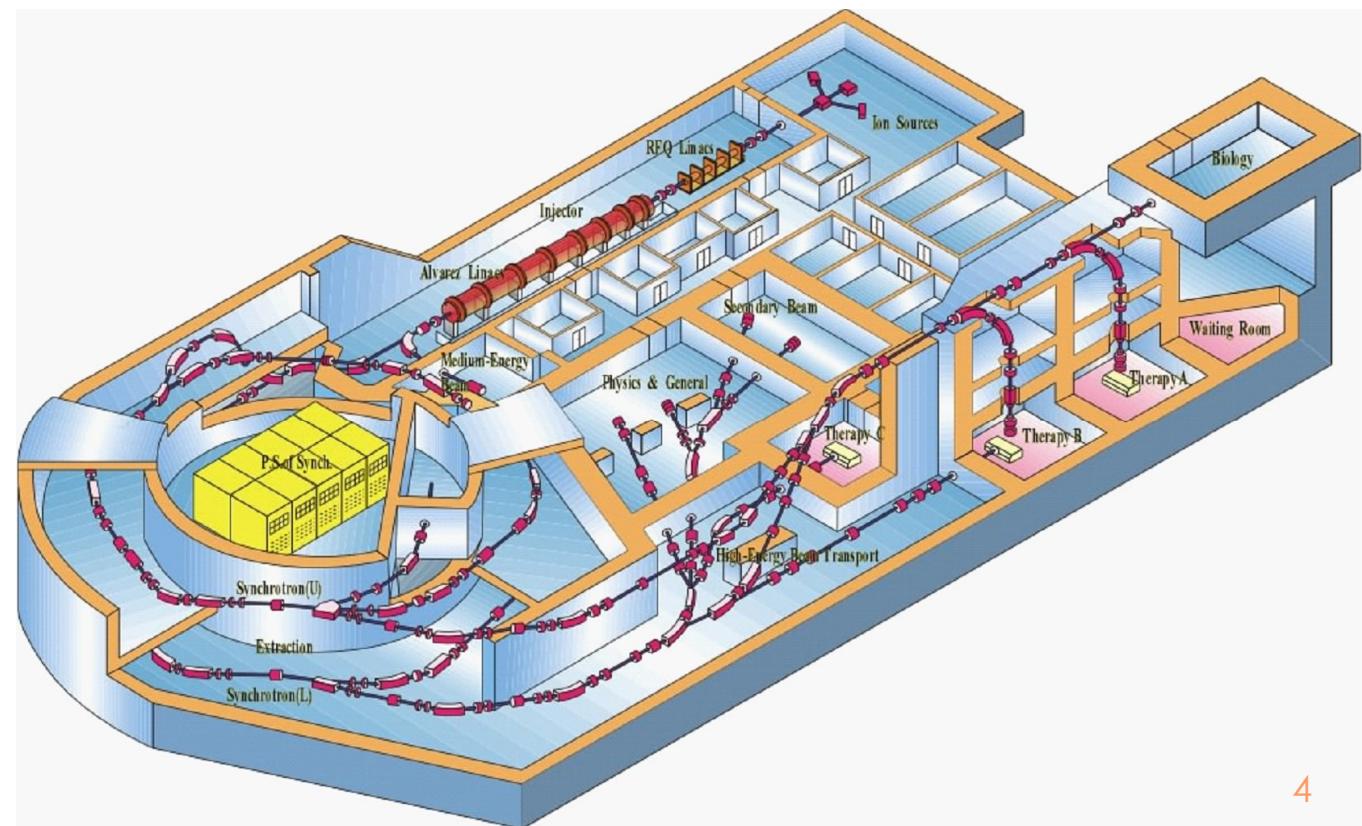


- **Introduction**
- **Gantry developments**
 - Superconducting magnets
 - Construction of gantry structure
- **Summary**

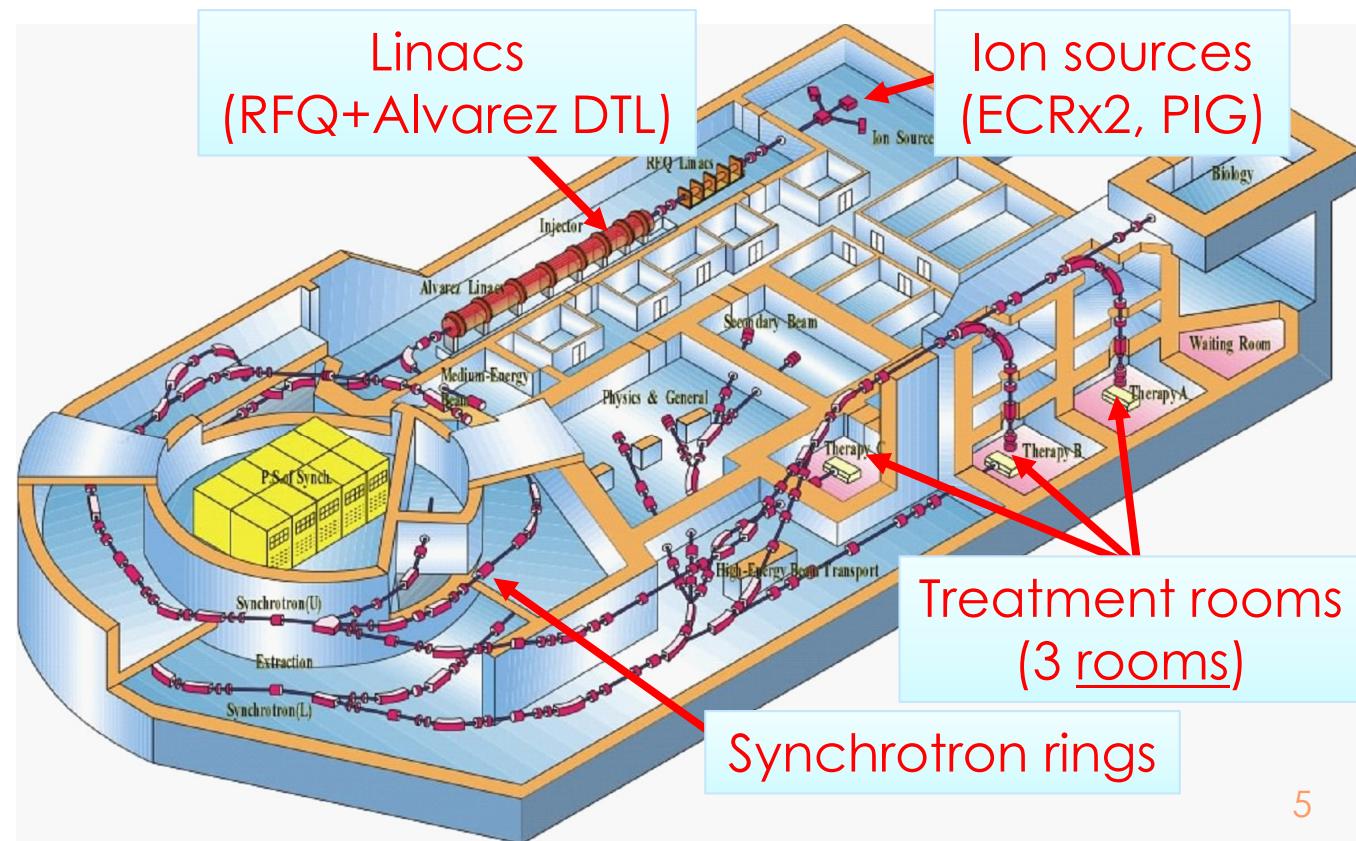


Introduction

Carbon radiotherapy



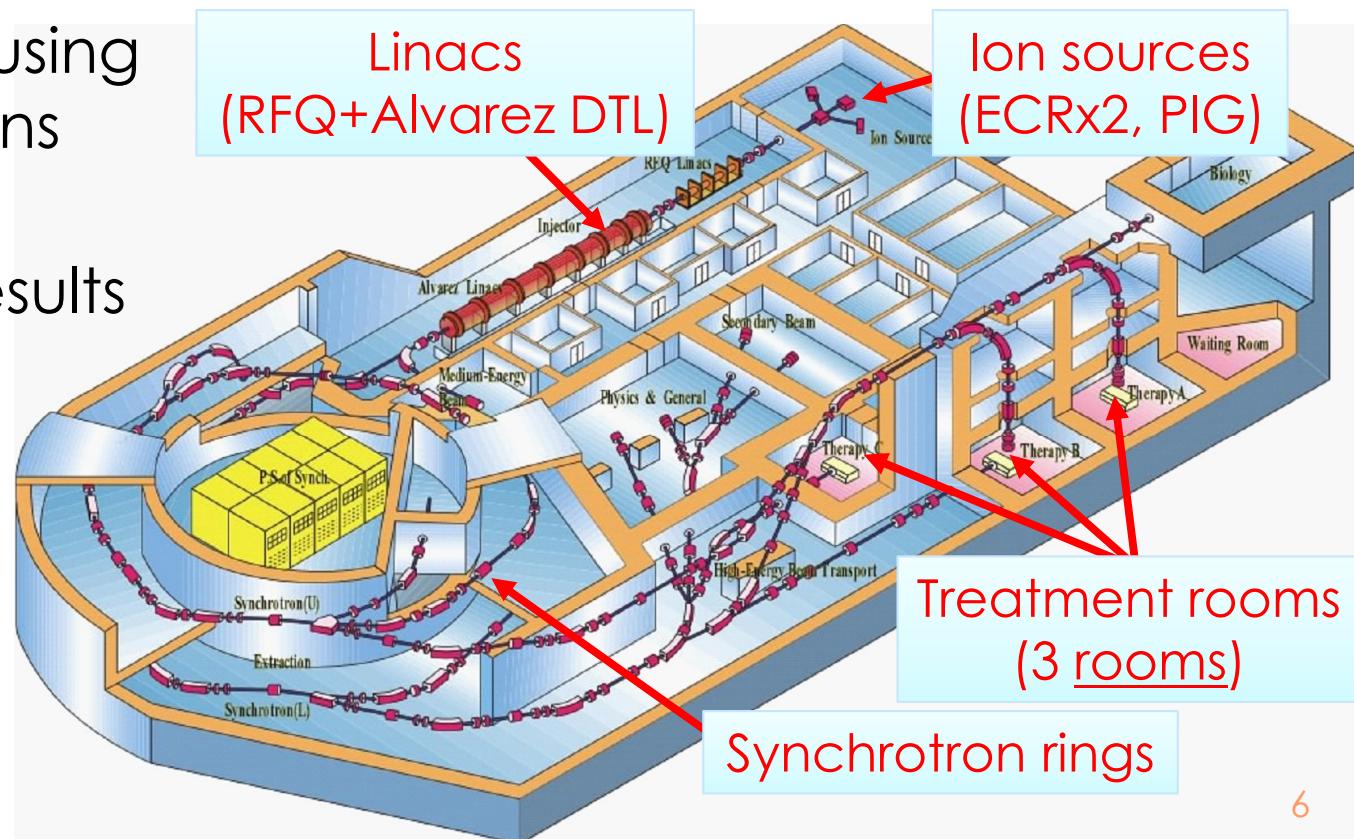
Carbon radiotherapy



Carbon radiotherapy



- Heavy Ion Medical Accelerator in Chiba (HIMAC)
- Ion species: p ~ Xe
- E/A=800 MeV for q/m=1/2
- Cancer treatments using energetic carbon ions since 1994
- Successful clinical results
~9000 patients



New treatment facility



- Construction completed in FY2010

- 3 treatment rooms

- Room E & F

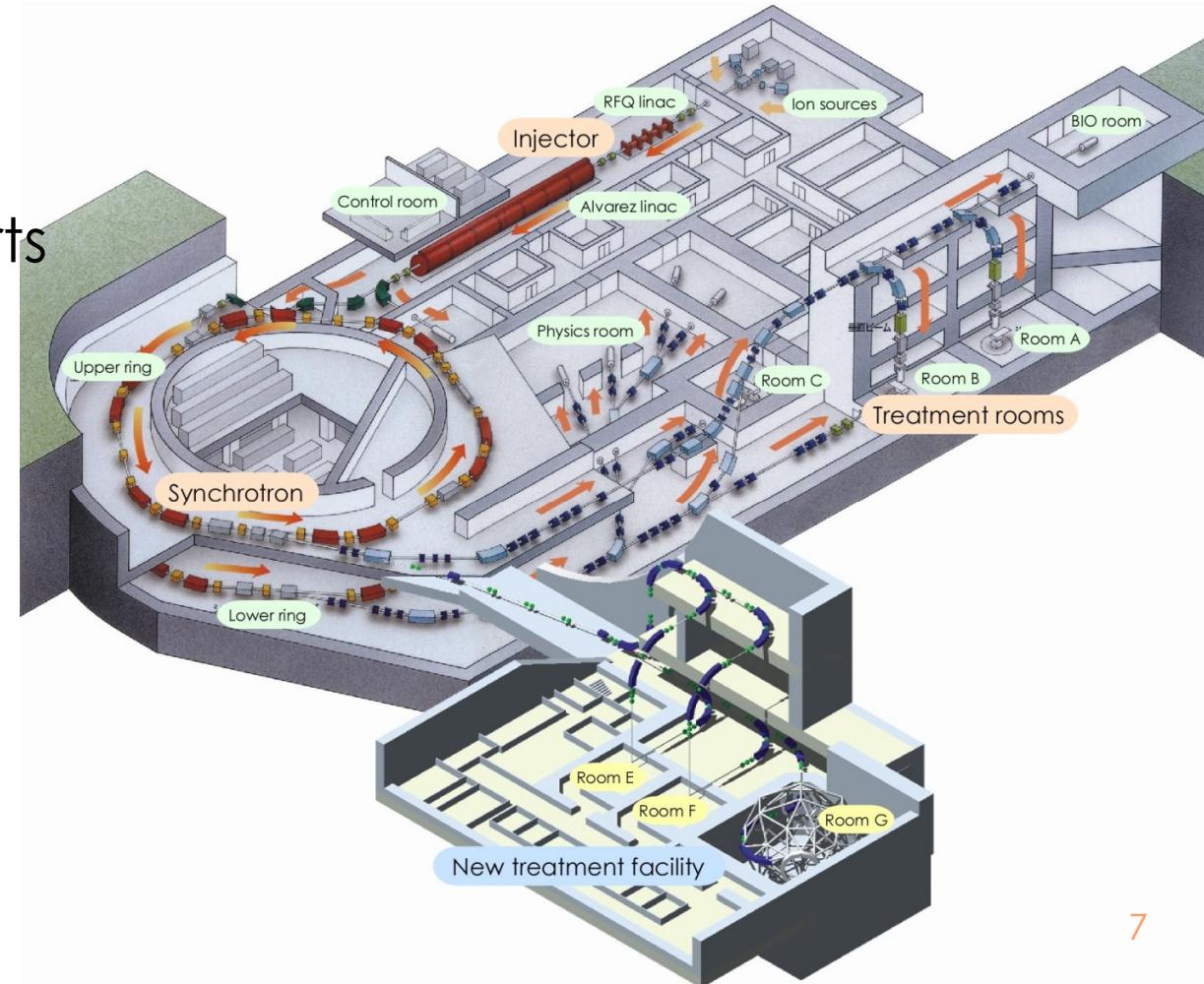
Fixed H&V scanning ports

(in treatment operation)

- **Room G**

Rotating gantry port

(Under construction)



New treatment facility



- Construction completed in FY2010

- 3 treatment rooms

- Room E & F

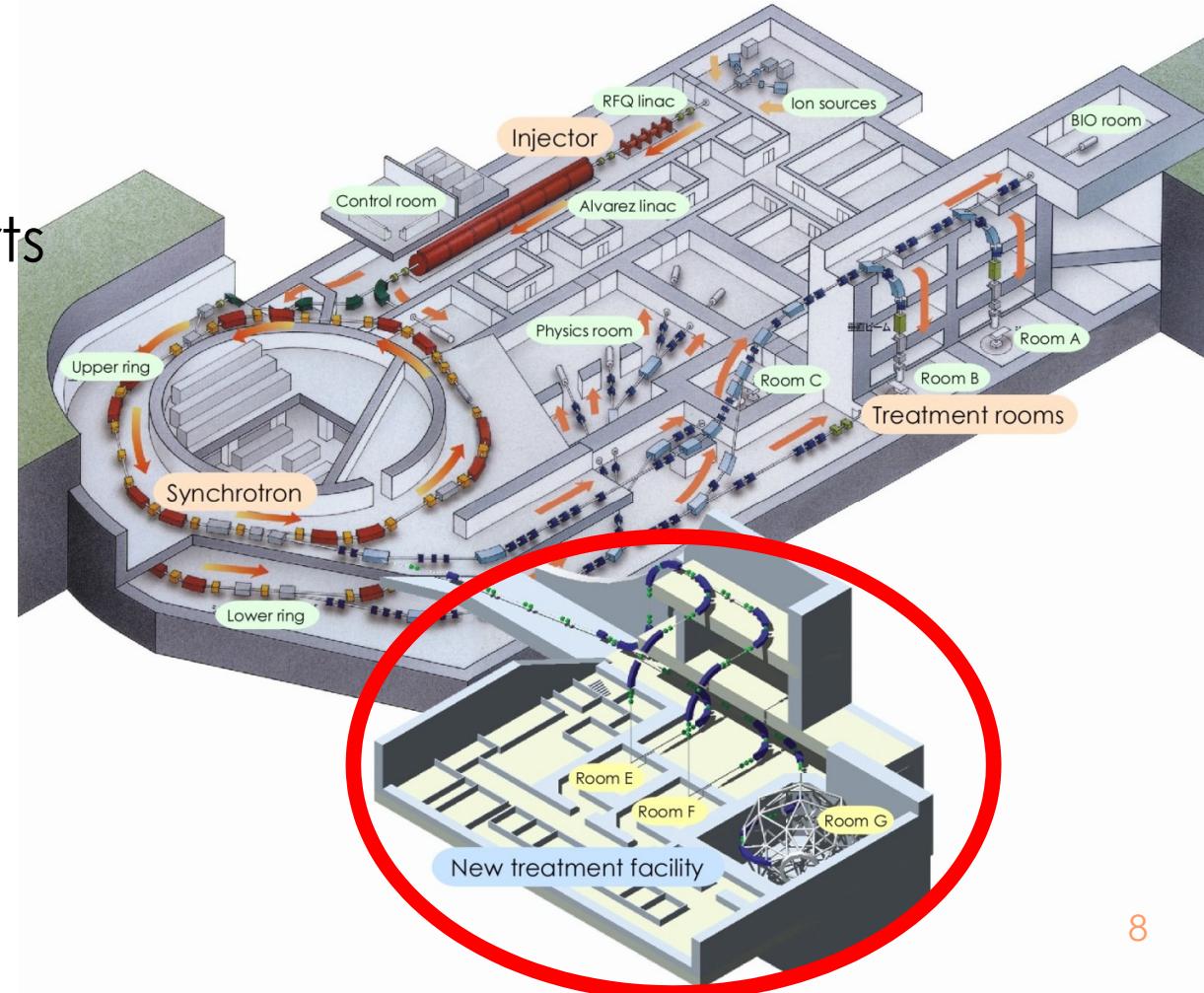
Fixed H&V scanning ports

(in treatment operation)

- Room G

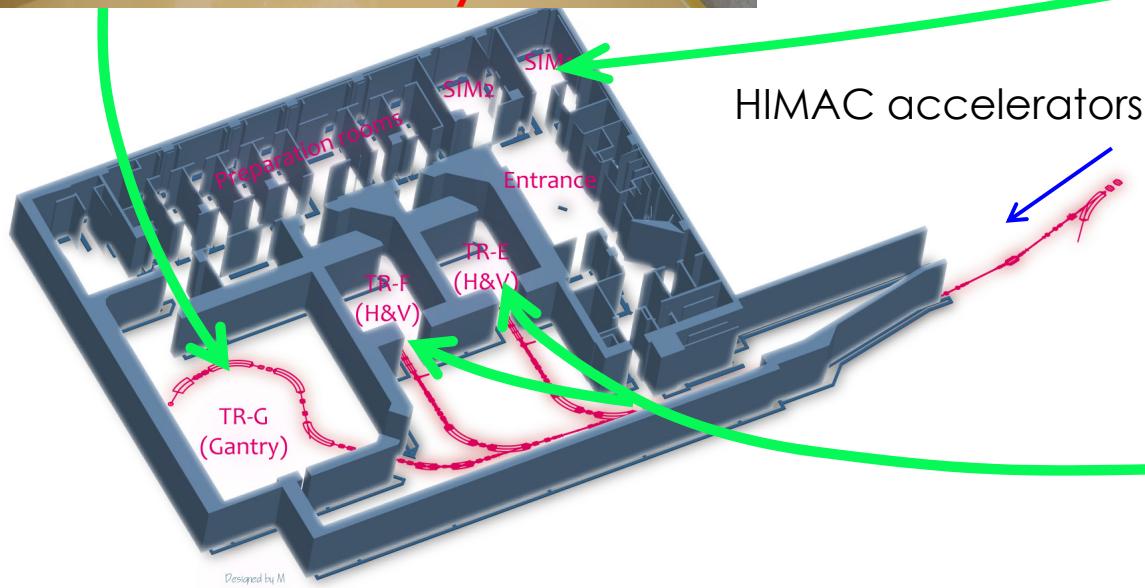
Rotating gantry port

(Under construction)





Treatment floor (B2F)



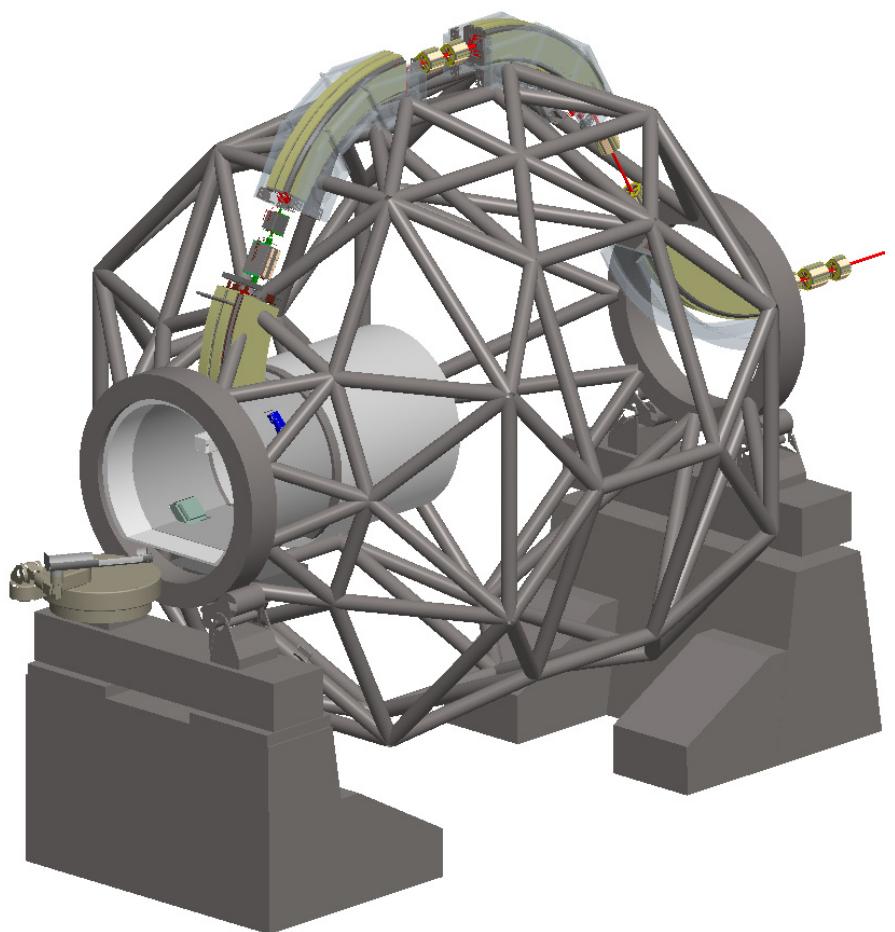


Rotating gantry in hadron radiotherapy

Needs for a rotating gantry



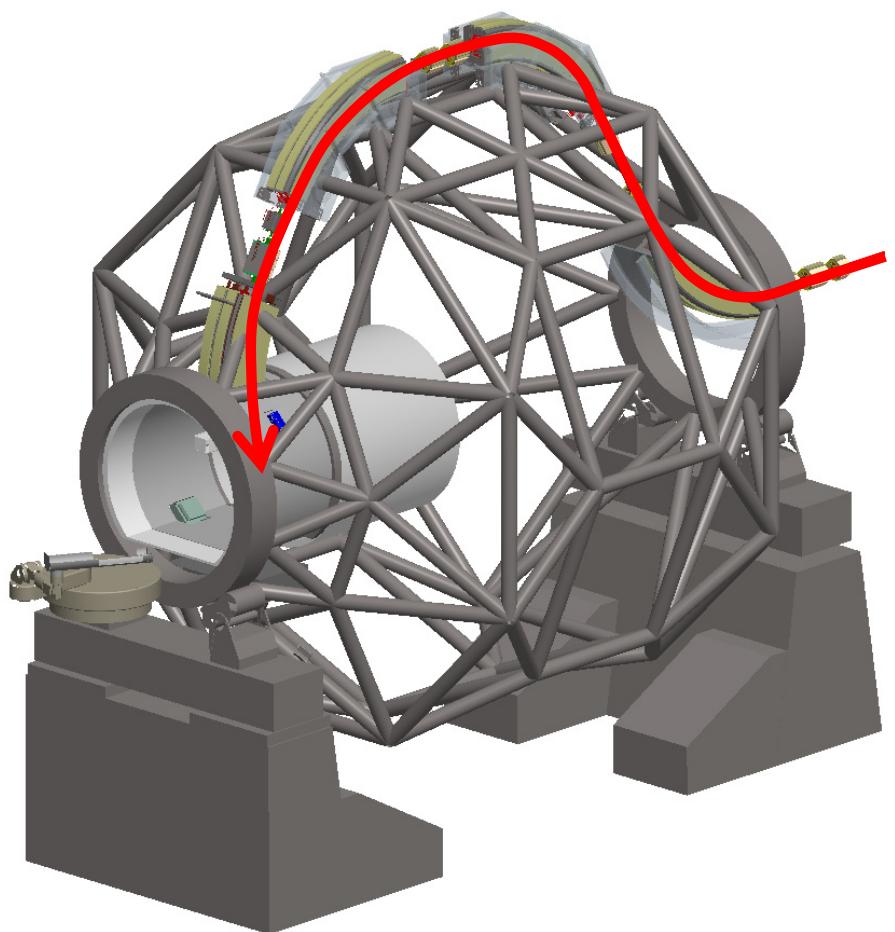
Irradiation with the existing fixed port



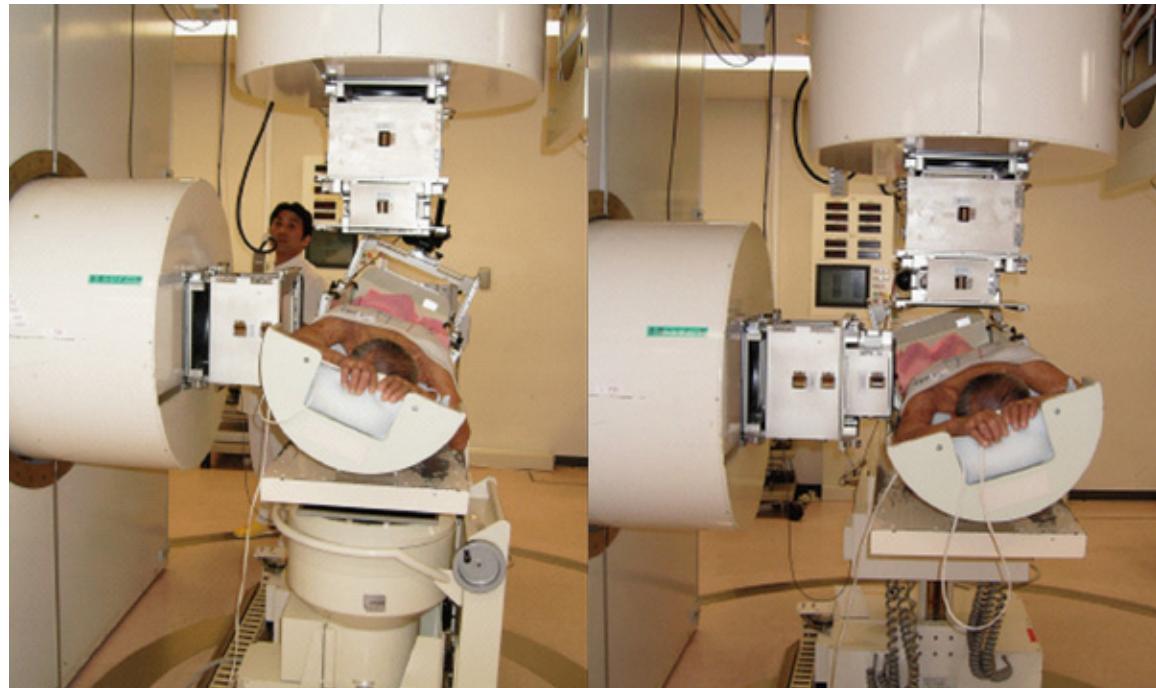
Needs for a rotating gantry



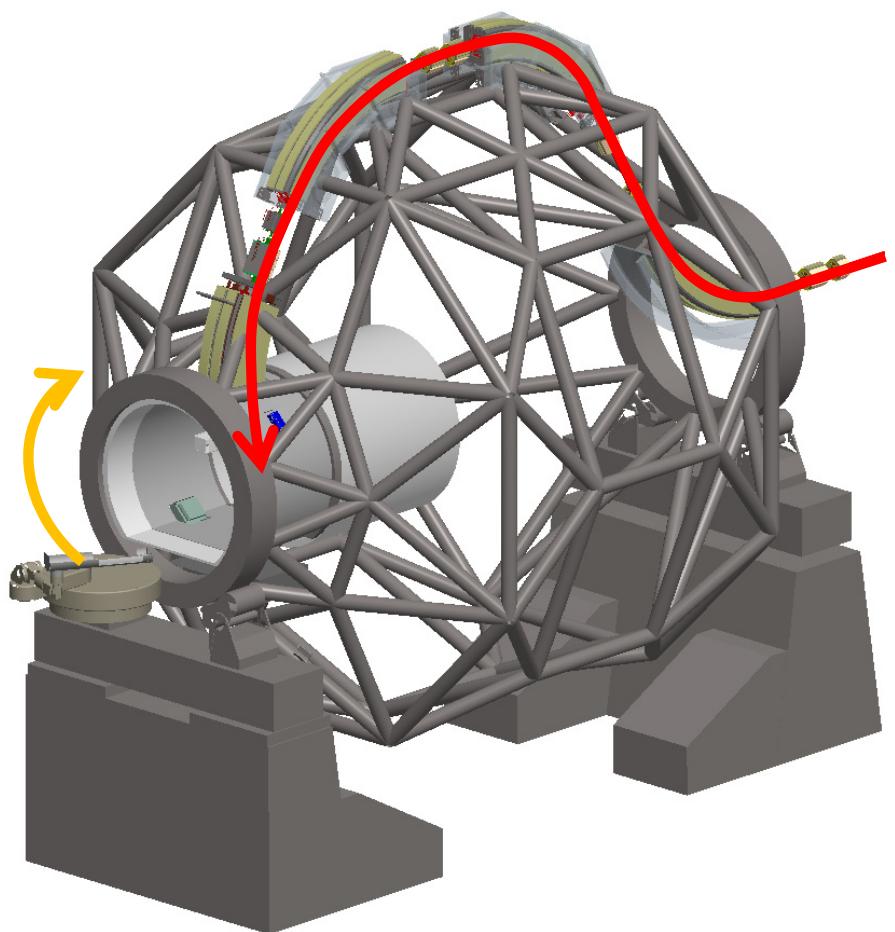
Irradiation with the existing fixed port



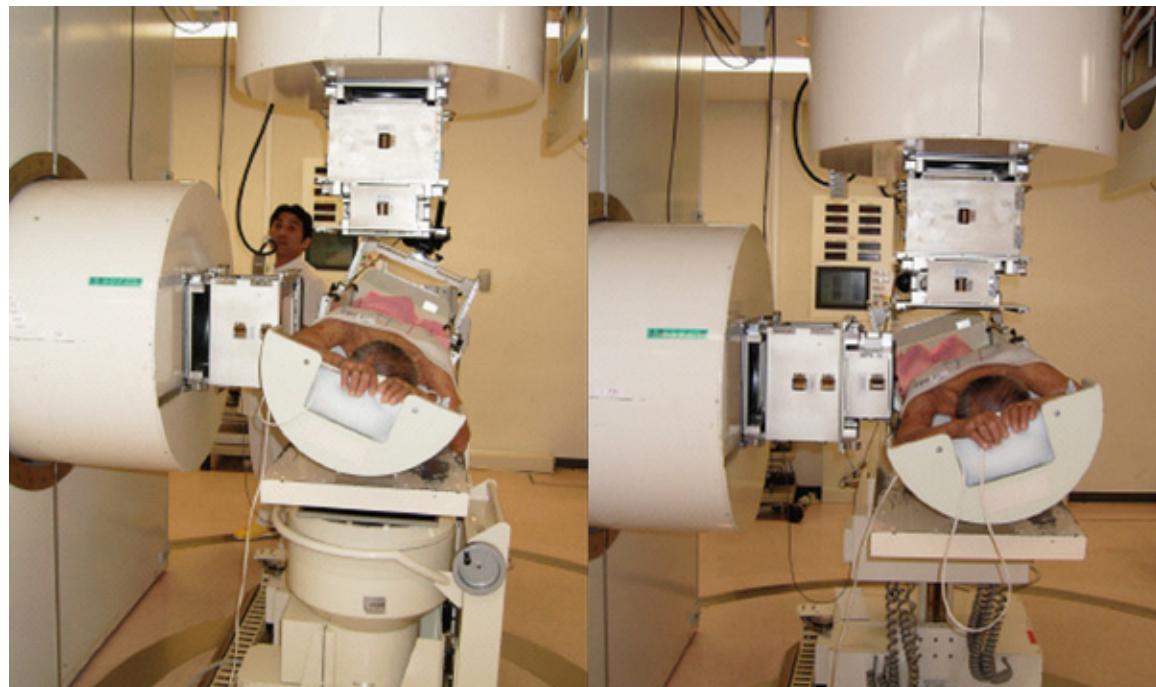
Needs for a rotating gantry



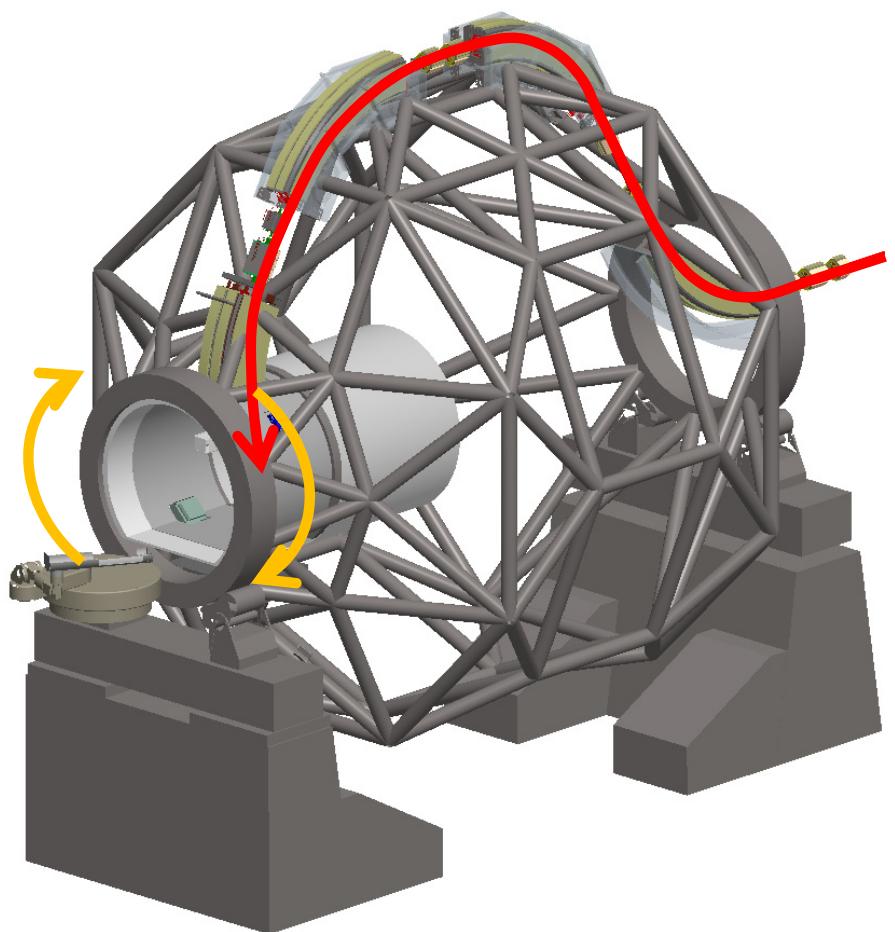
Irradiation with the existing fixed port



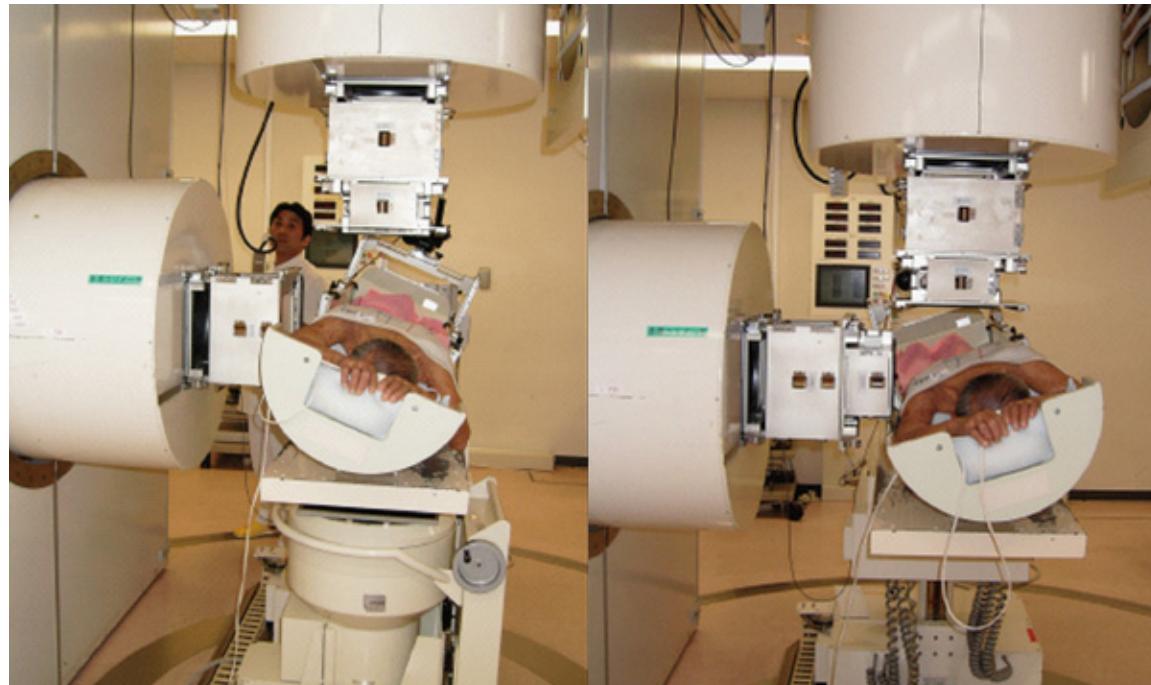
Needs for a rotating gantry



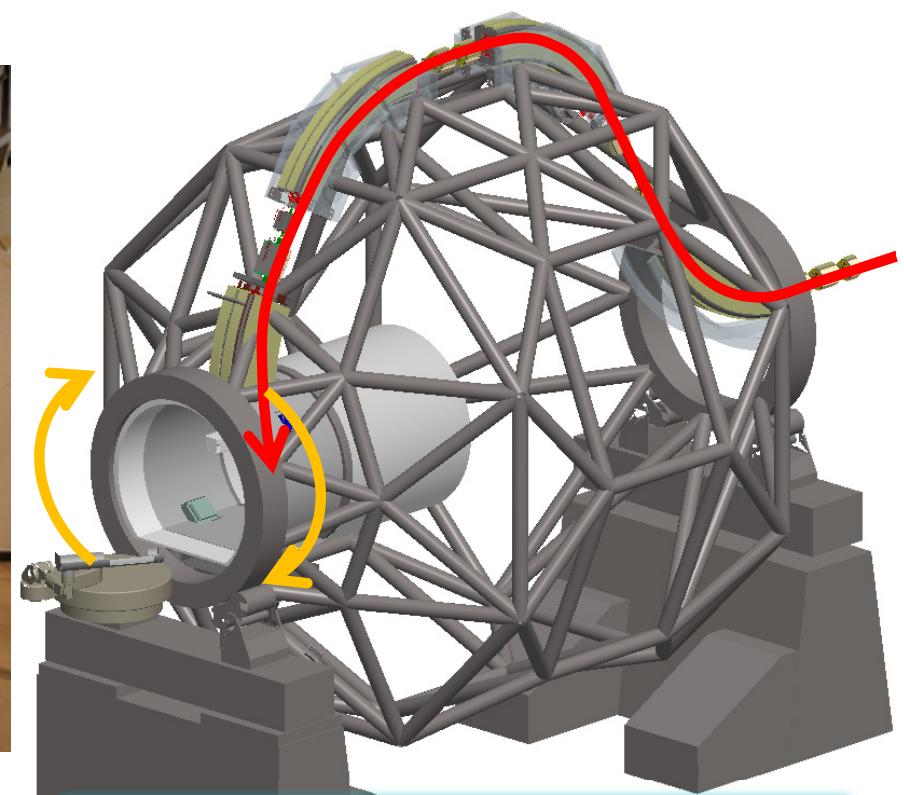
Irradiation with the existing fixed port



Needs for a rotating gantry



Irradiation with the existing fixed port



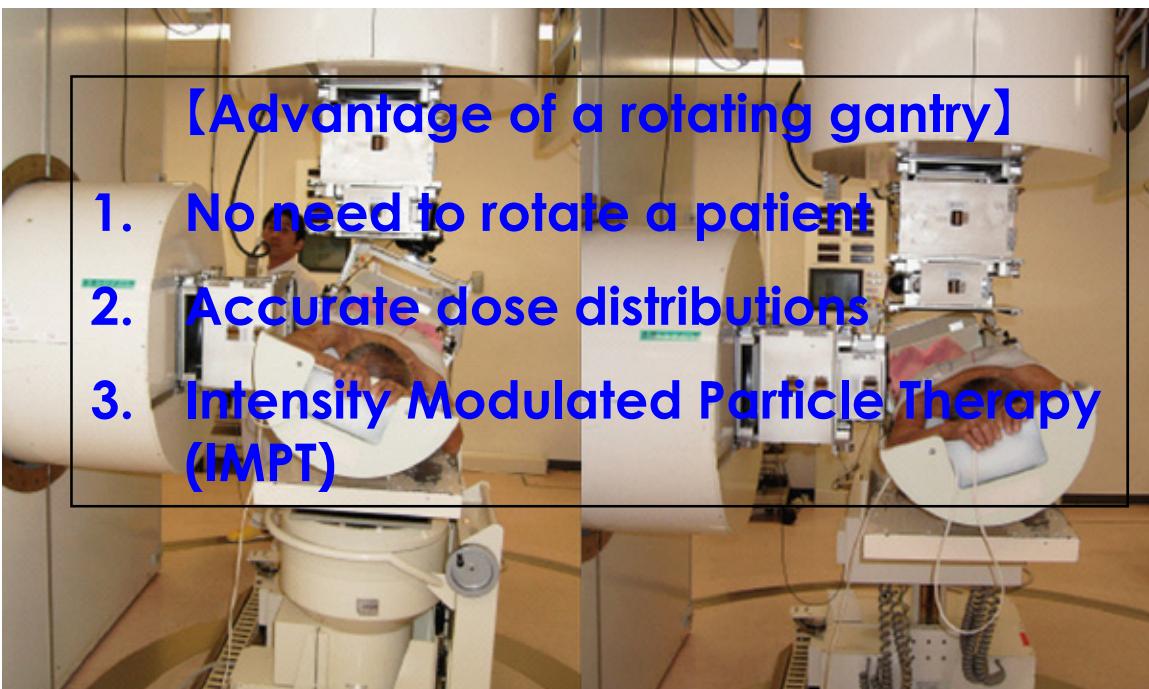
Beam can be directed to a target from **any** of medically desirable angles

Needs for a rotating gantry

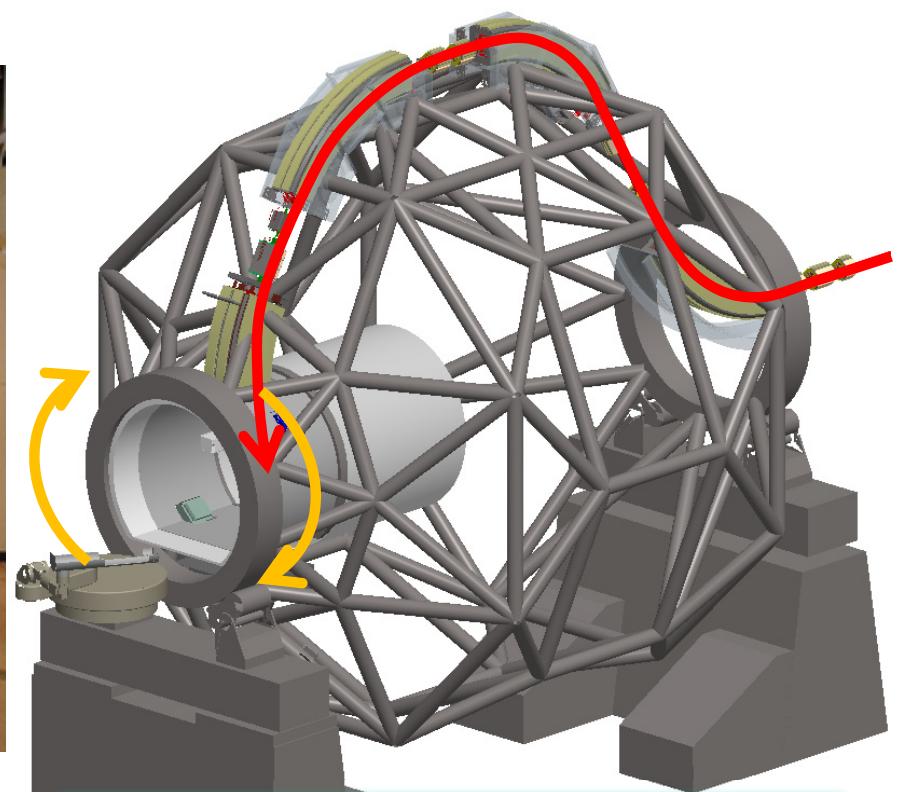


[Advantage of a rotating gantry]

1. No need to rotate a patient
2. Accurate dose distributions
3. Intensity Modulated Particle Therapy (IMPT)



Irradiation with the existing fixed port



Beam can be directed to a target from **any** of medically desirable angles

Rotating gantry for hadron therapy



- **Proton therapy**

- Gantry are commonly used
- Commercially available

- **Carbon therapy**

- Required B_p is 3 times higher
 - Magnets will be very large and heavy
- Difficult to
 - Design
 - Construct



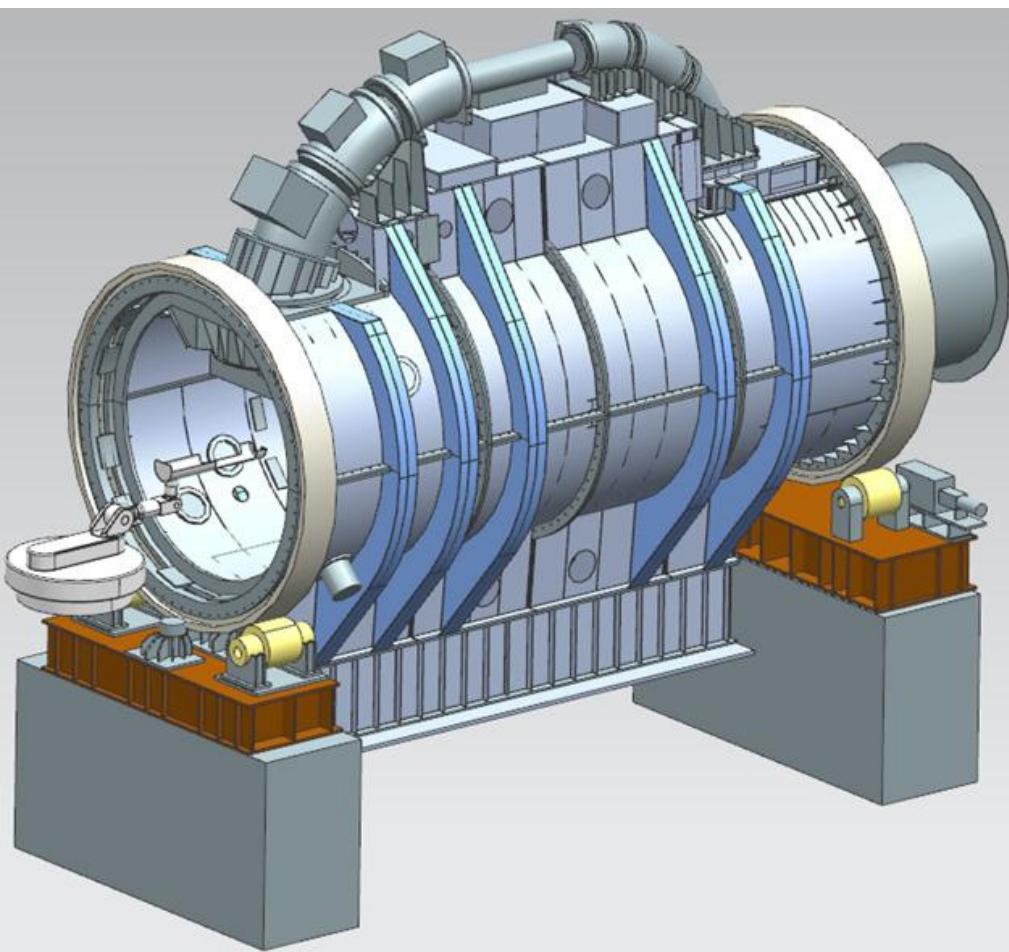
Rotating gantry for carbon therapy

- **Only one gantry in the world**
 - Heidelberg Ion Beam Therapy Center (HIT)
 - World first carbon-gantry
 - Clinical use since November 2012
 - Weight: 600 tons
(rotating part)



<http://idw-online.de/pages/de/news504069>

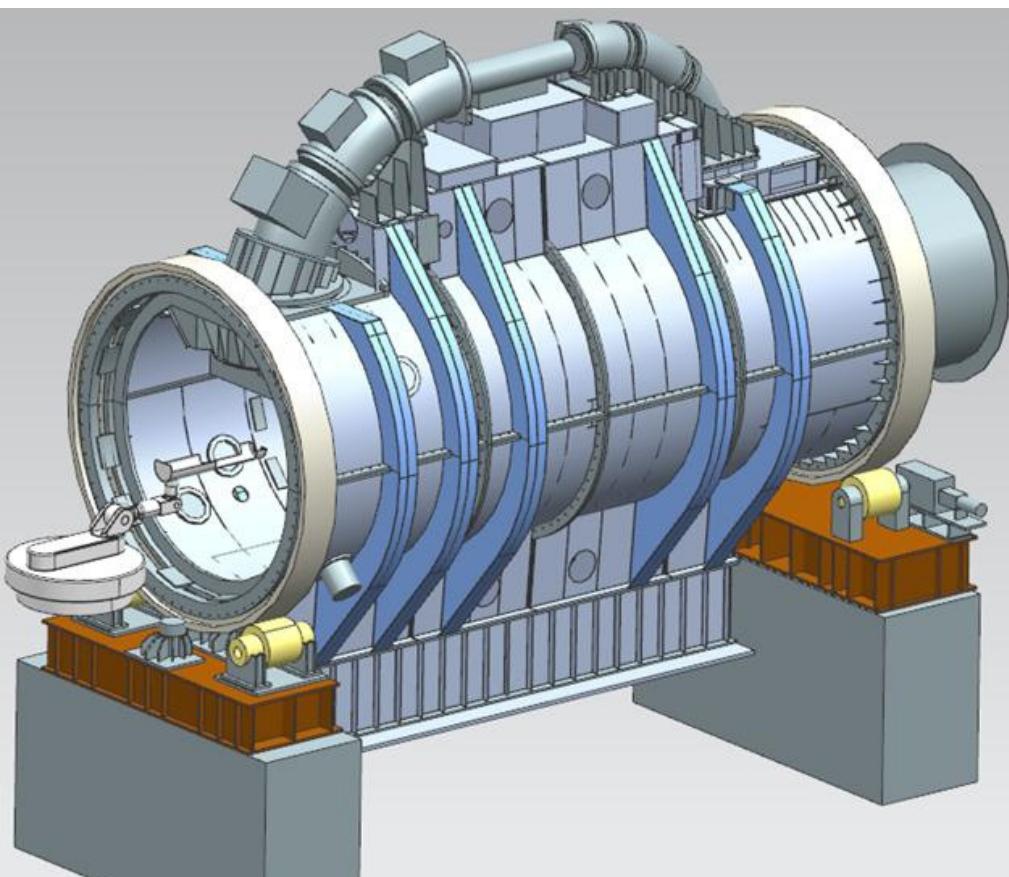
Superconducting rotating-gantry



Use of superconducting (SC) magnets

Ion kind	: ^{12}C
Irradiation method:	3D Scanning
Beam energy	: 430 MeV/n
Maximum range	: 30 cm in water
Scan size	: $\square 200 \times 200 \text{ mm}^2$
Beam orbit radius	: 5.45 m
Length	: 13 m

Superconducting rotating-gantry



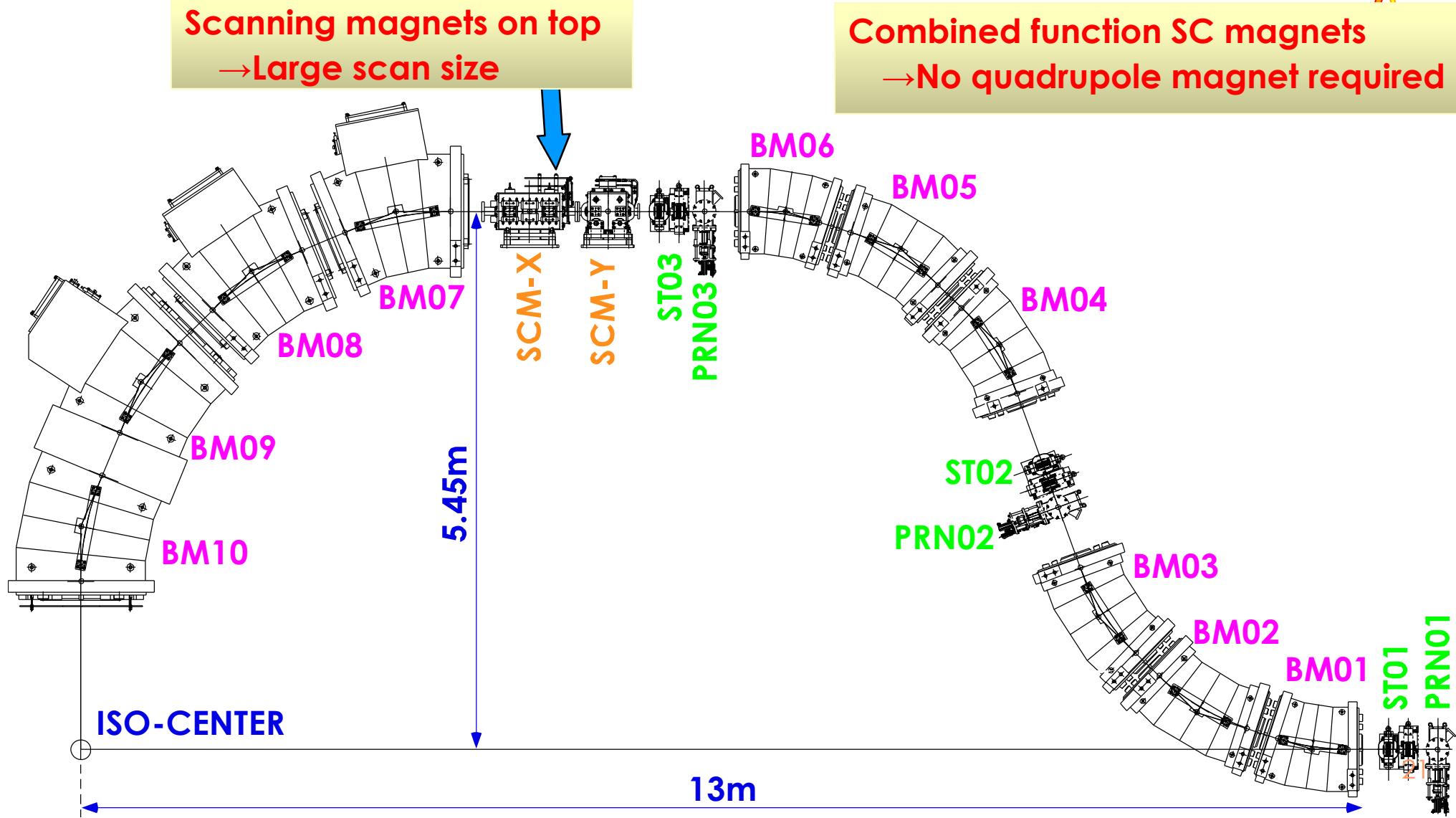
Weight: order of 300 tons

Use of superconducting (SC) magnets

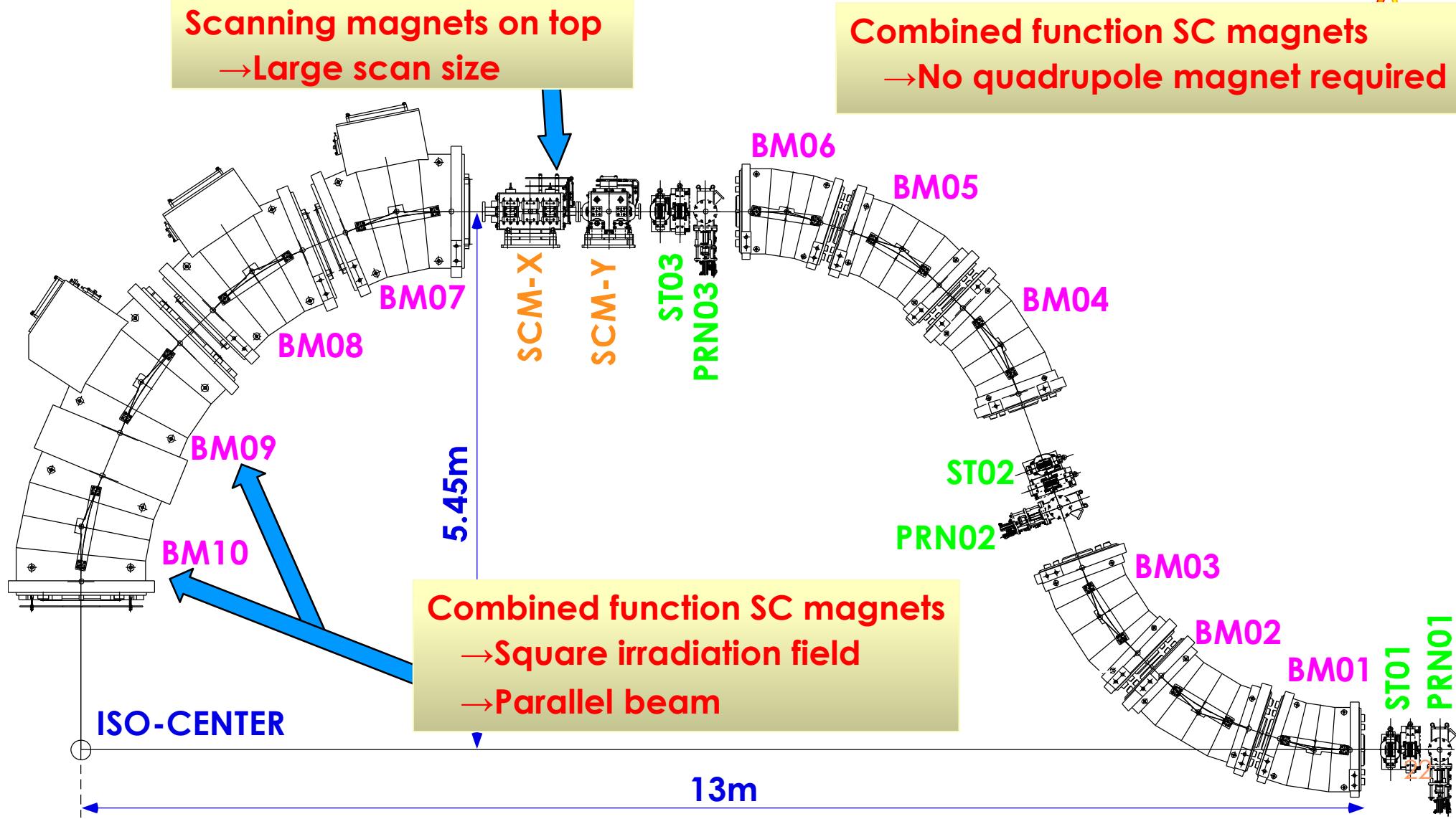
Ion kind	: ^{12}C
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Beam energy	: 430 MeV/n
Maximum range	: 30 cm in water
Scan size	: $\square 200 \times 200 \text{ mm}^2$
Beam orbit radius	: 5.45 m
Length	: 13 m

The size and weight are considerably reduced

Layout of the SC gantry



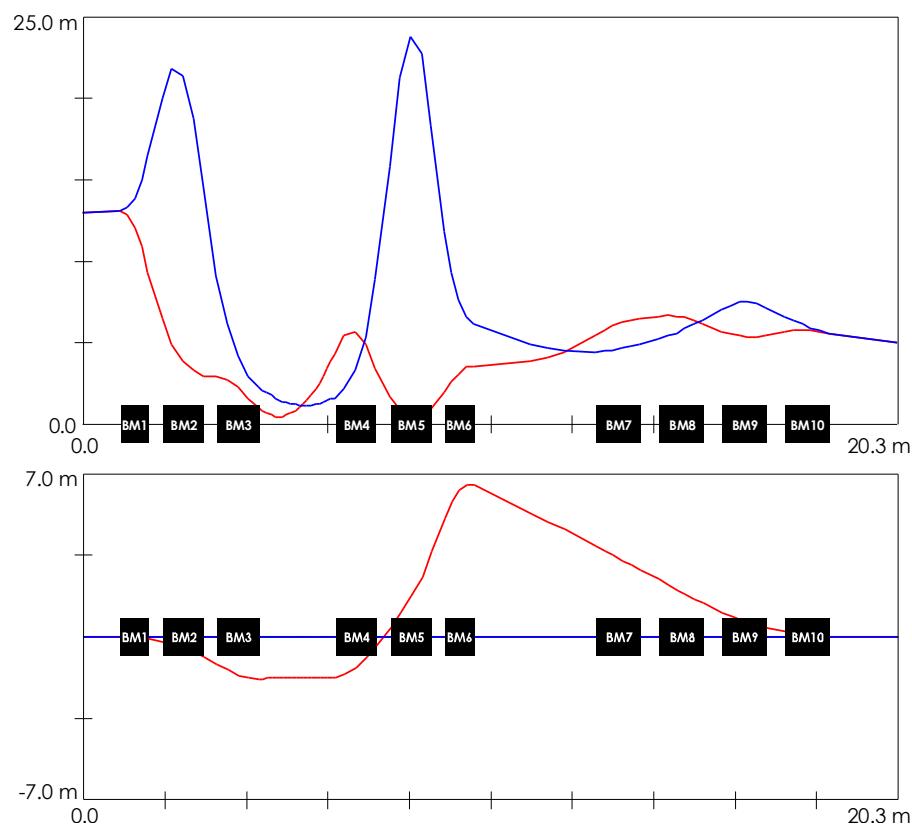
Layout of the SC gantry



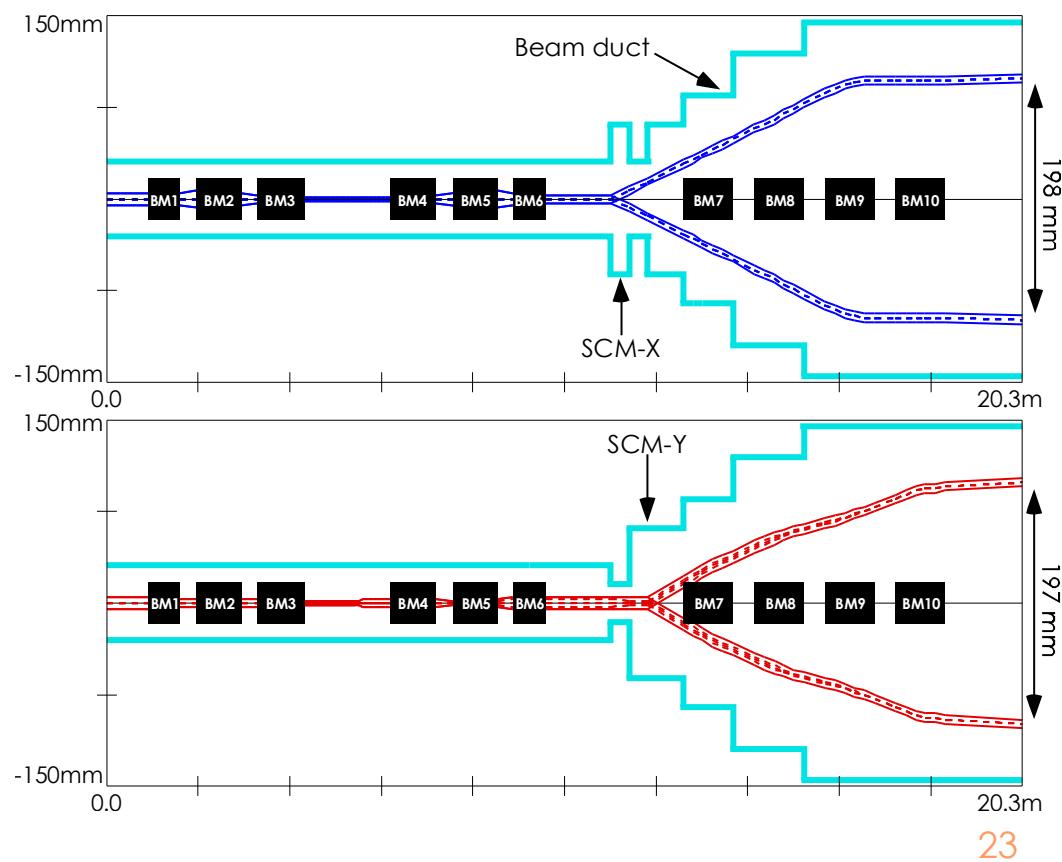
Beam optics design



Beta and dispersion functions



Beam envelope functions with kicks of scanning magnets



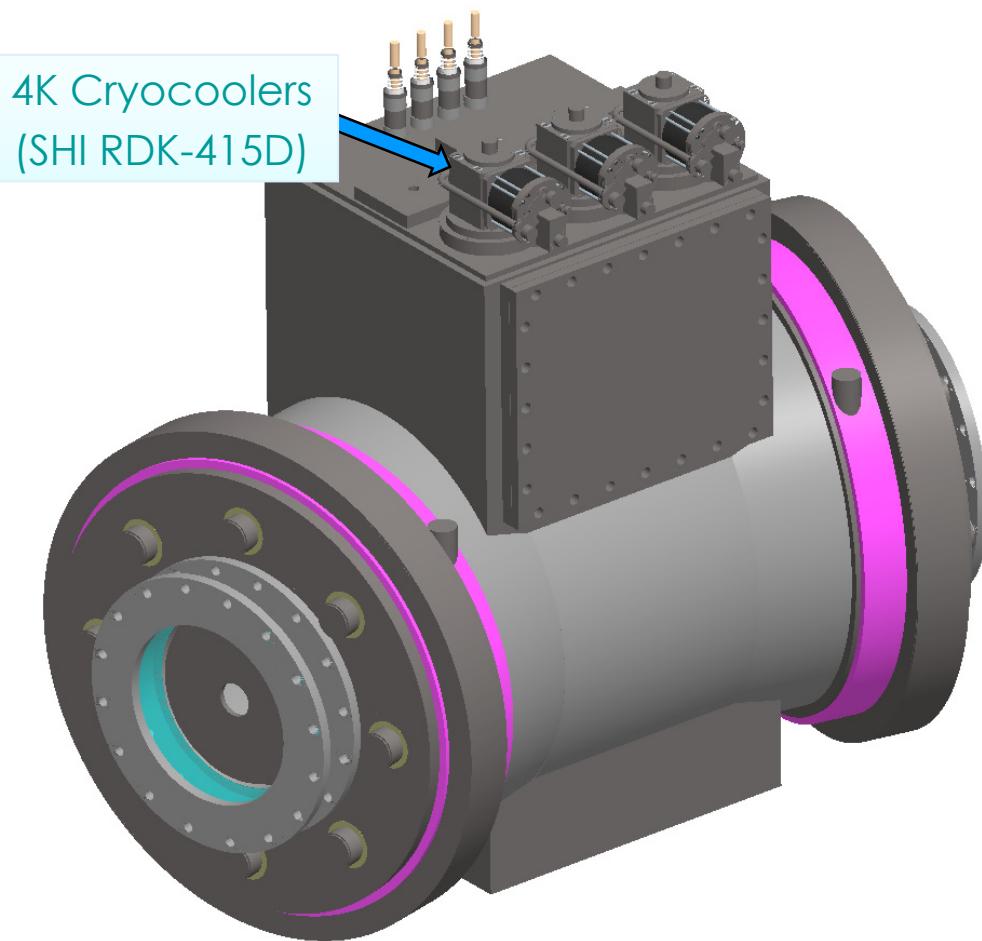


Development of superconducting magnets

Development of curved SC magnets



SC magnet (BM02-05)

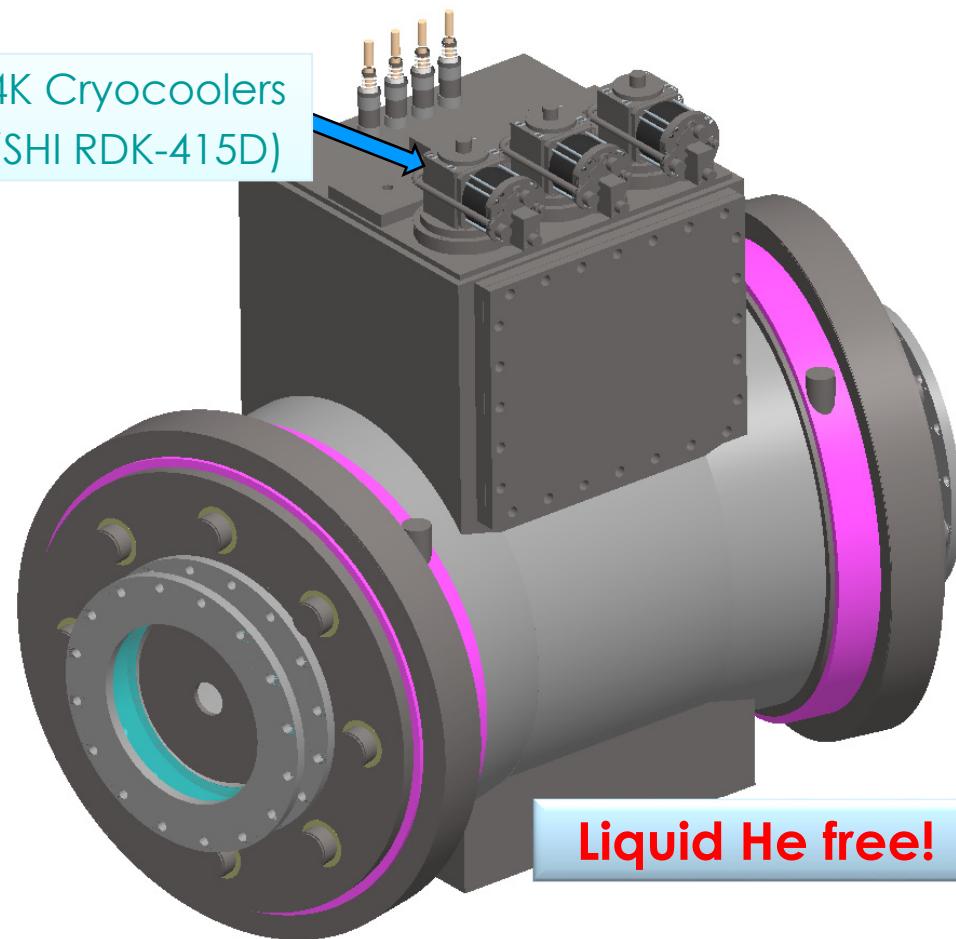


4K Cryocoolers
(SHI RDK-415D)

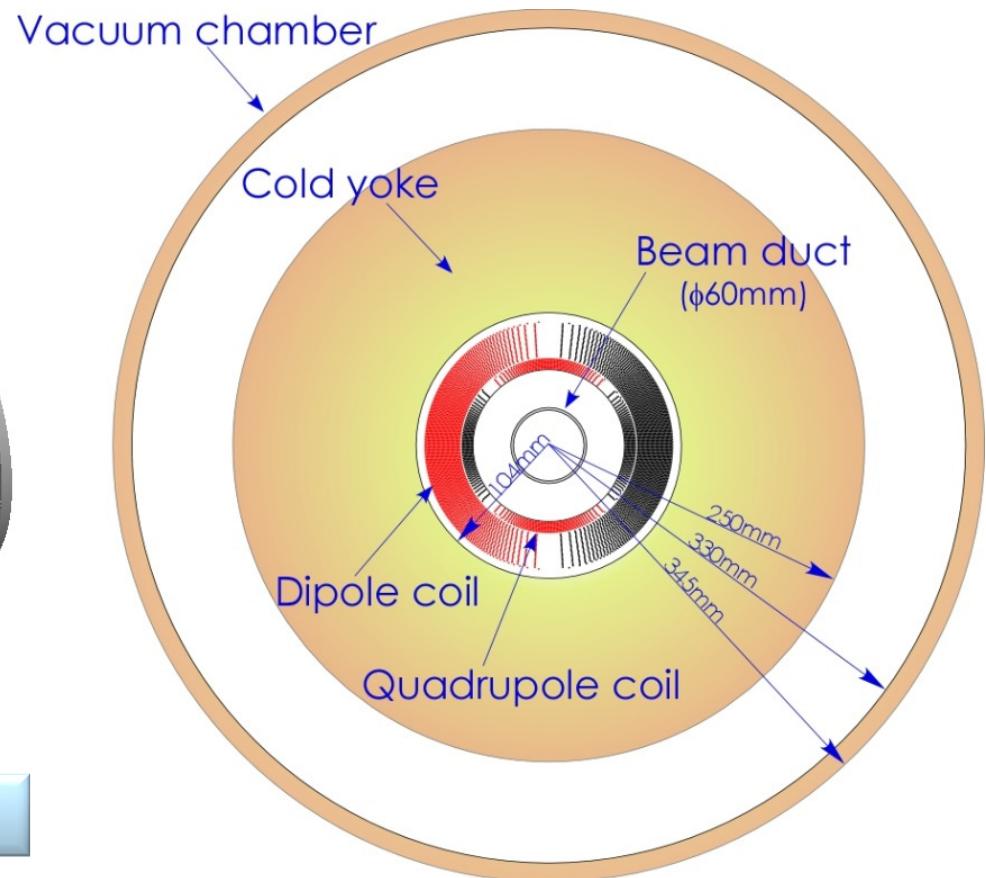
Development of curved SC magnets



SC magnet (BM02-05)

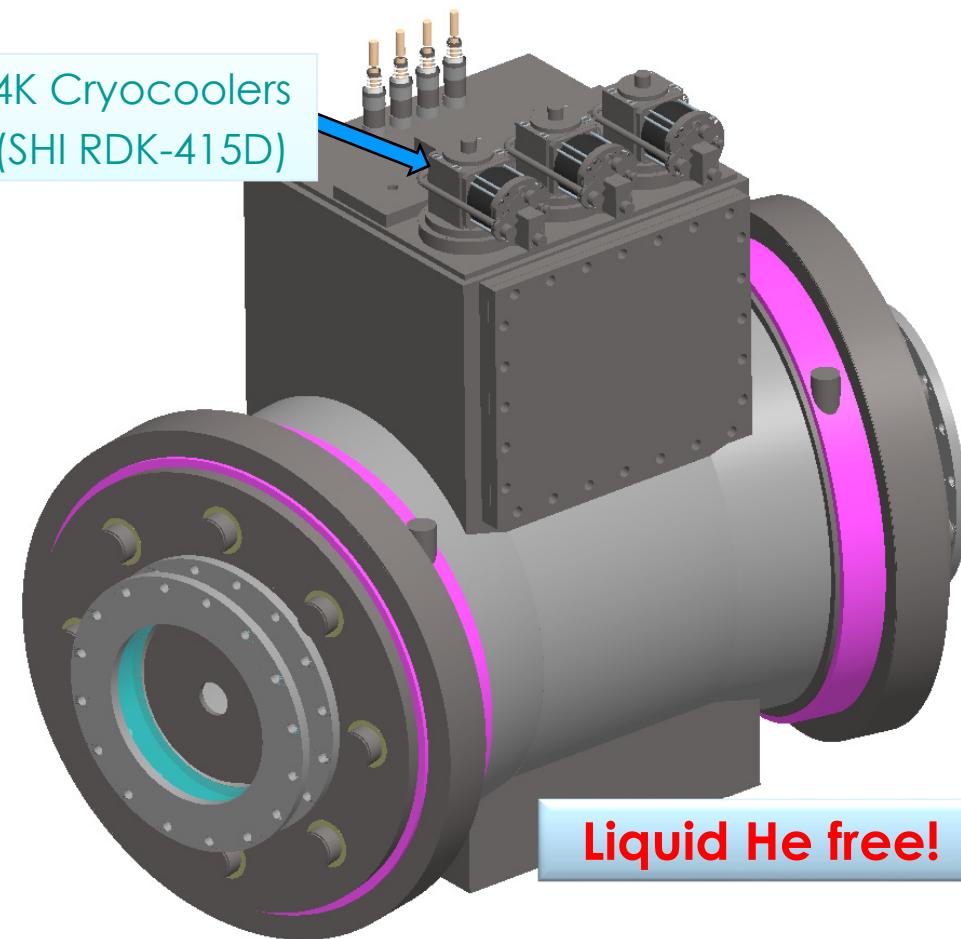


Cross-sectional view

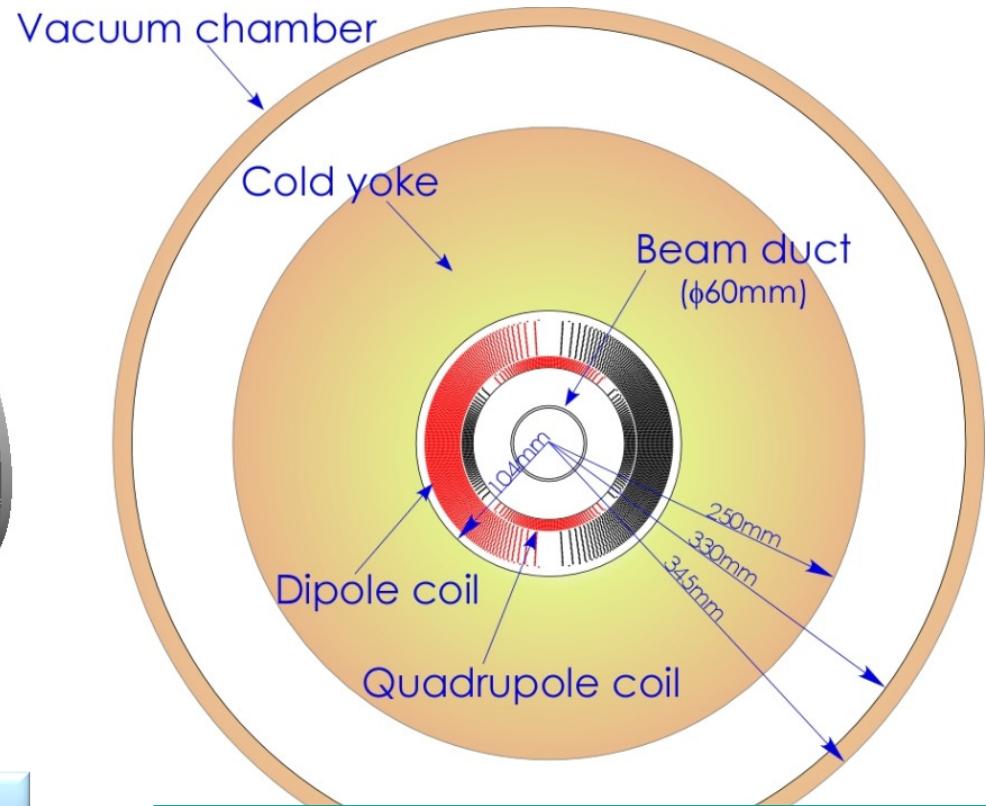


Development of curved SC magnets

SC magnet (BM02-05)



Cross-sectional view

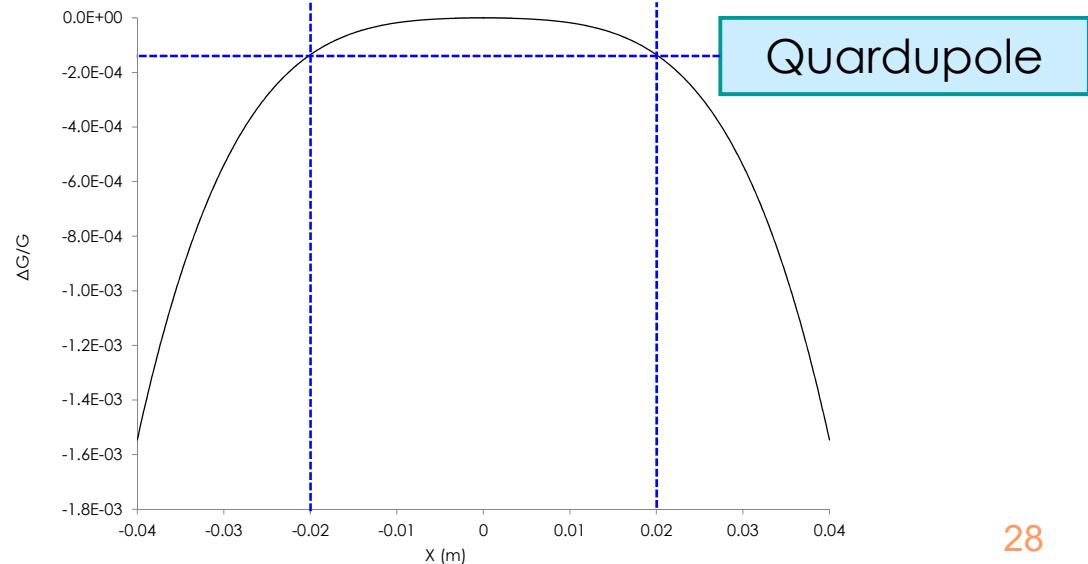
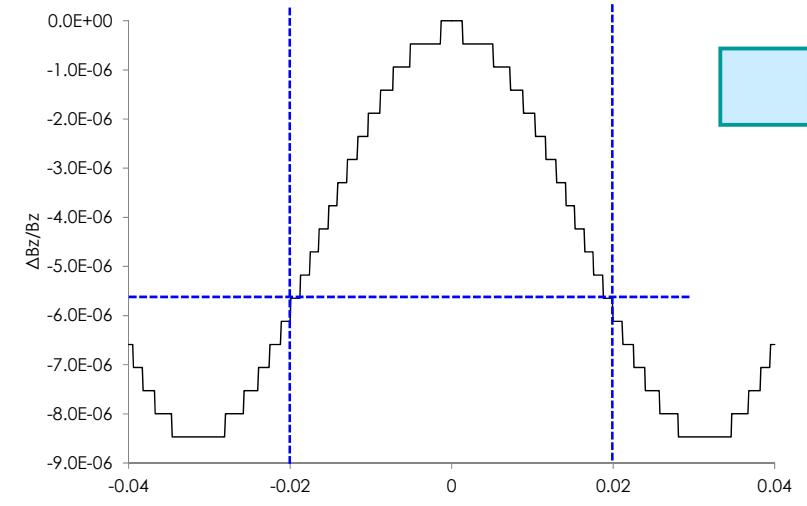
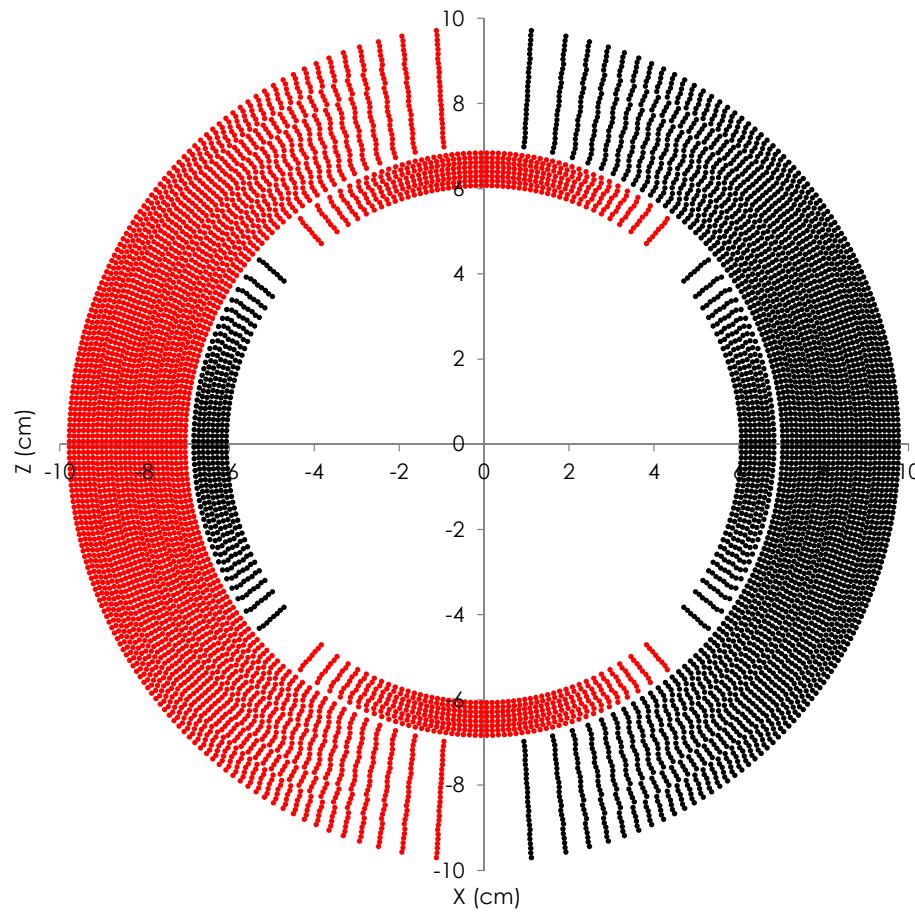


Dipole and quadrupole coils can be independently excited

Design of superconducting coils



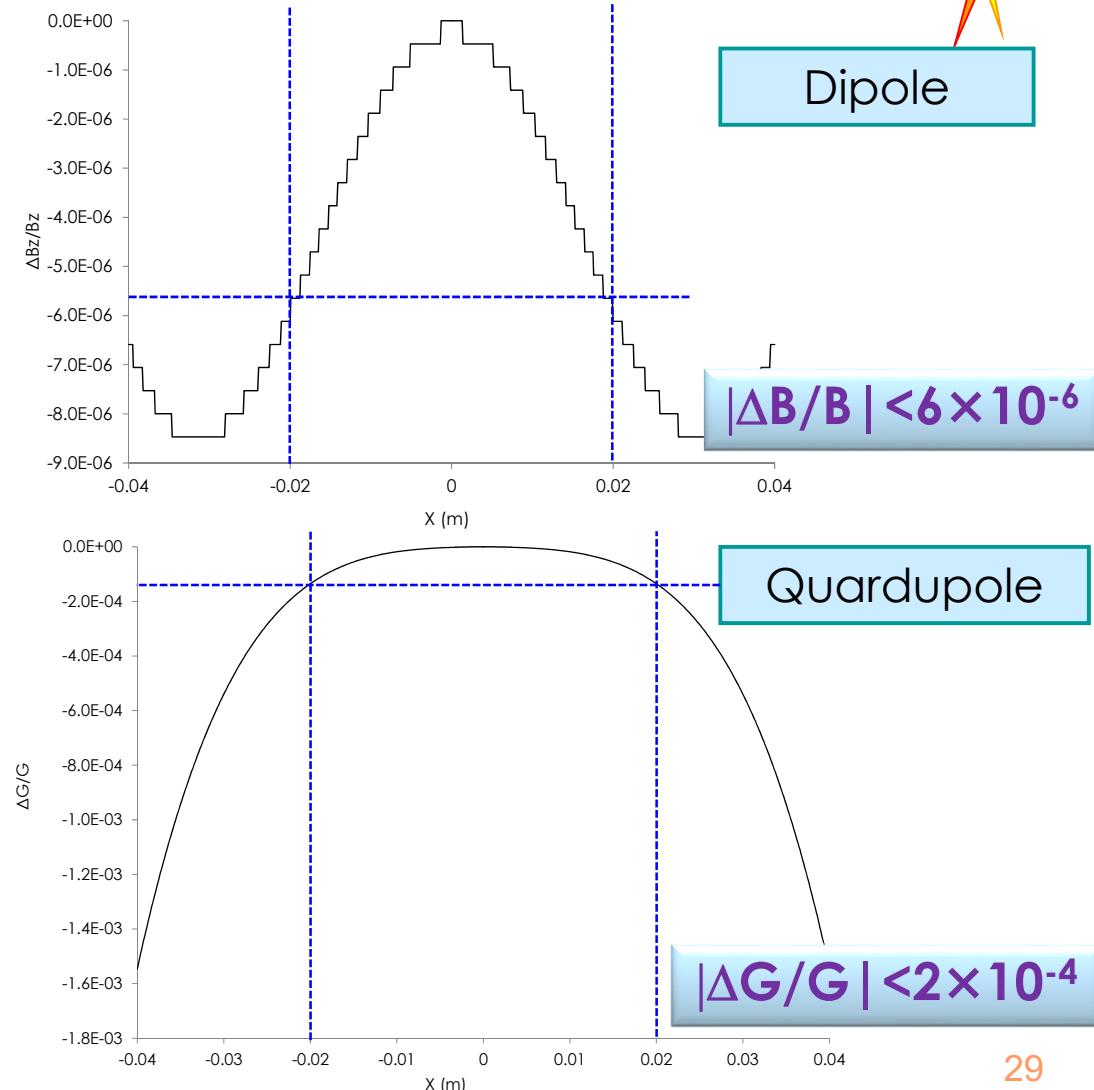
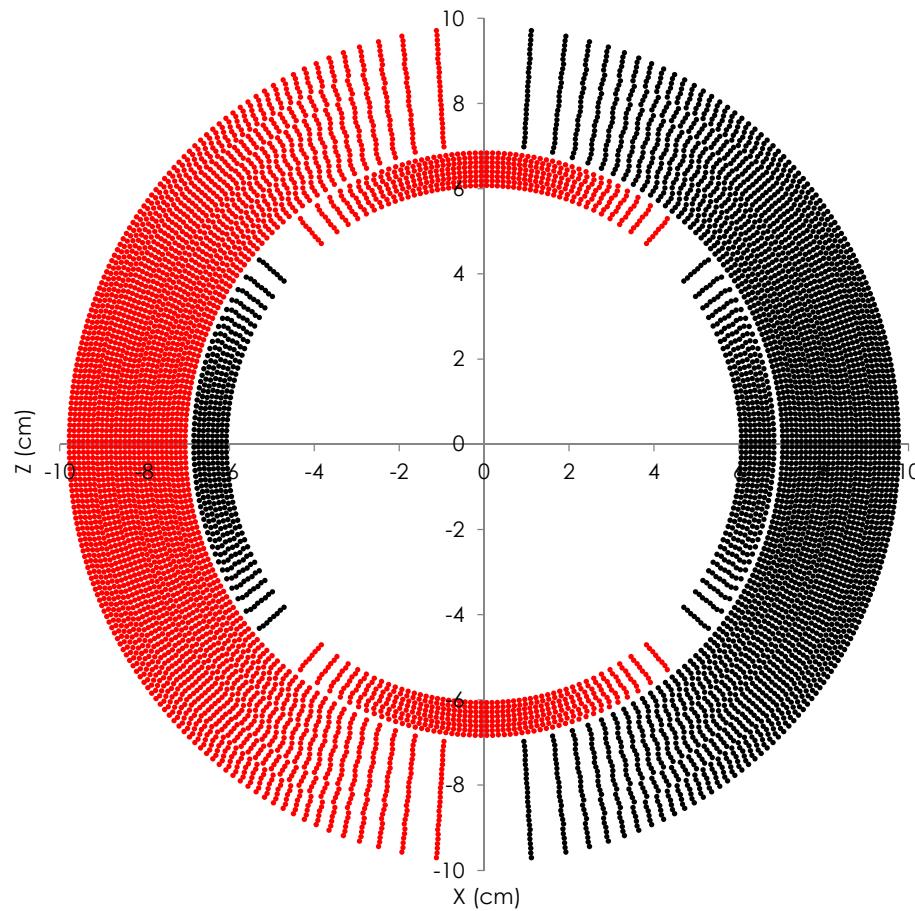
2D field calculation
(BM02-BM05)



Design of superconducting coils



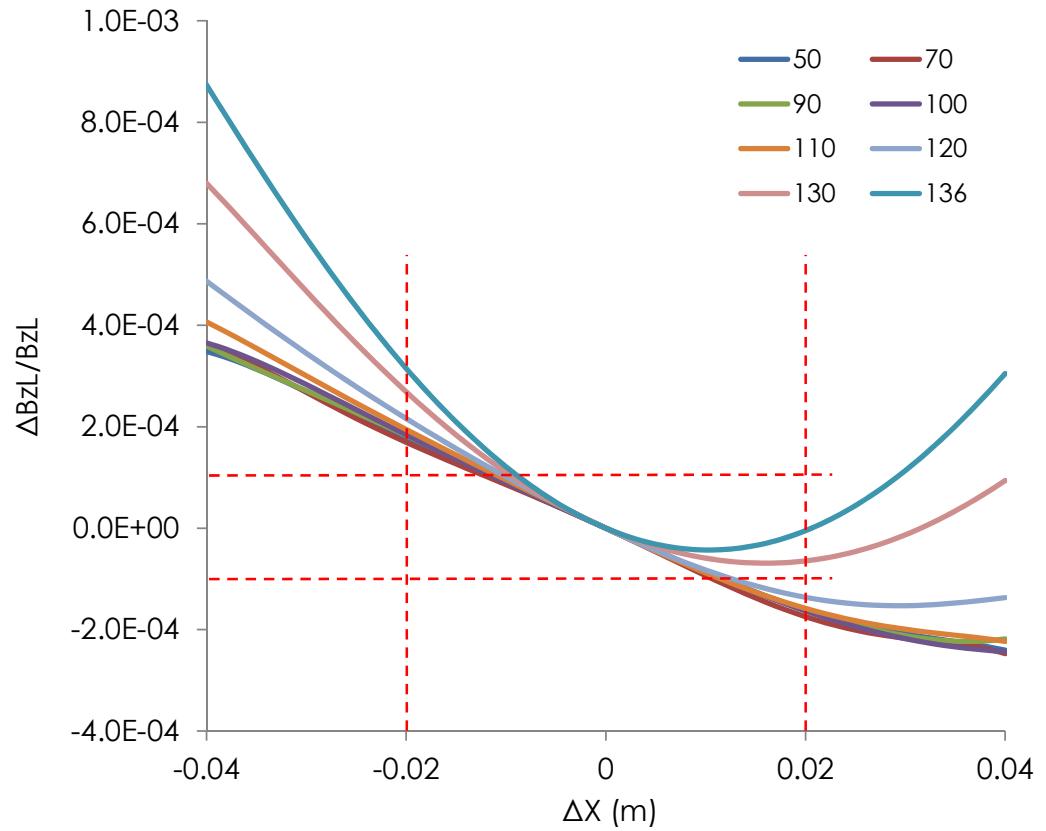
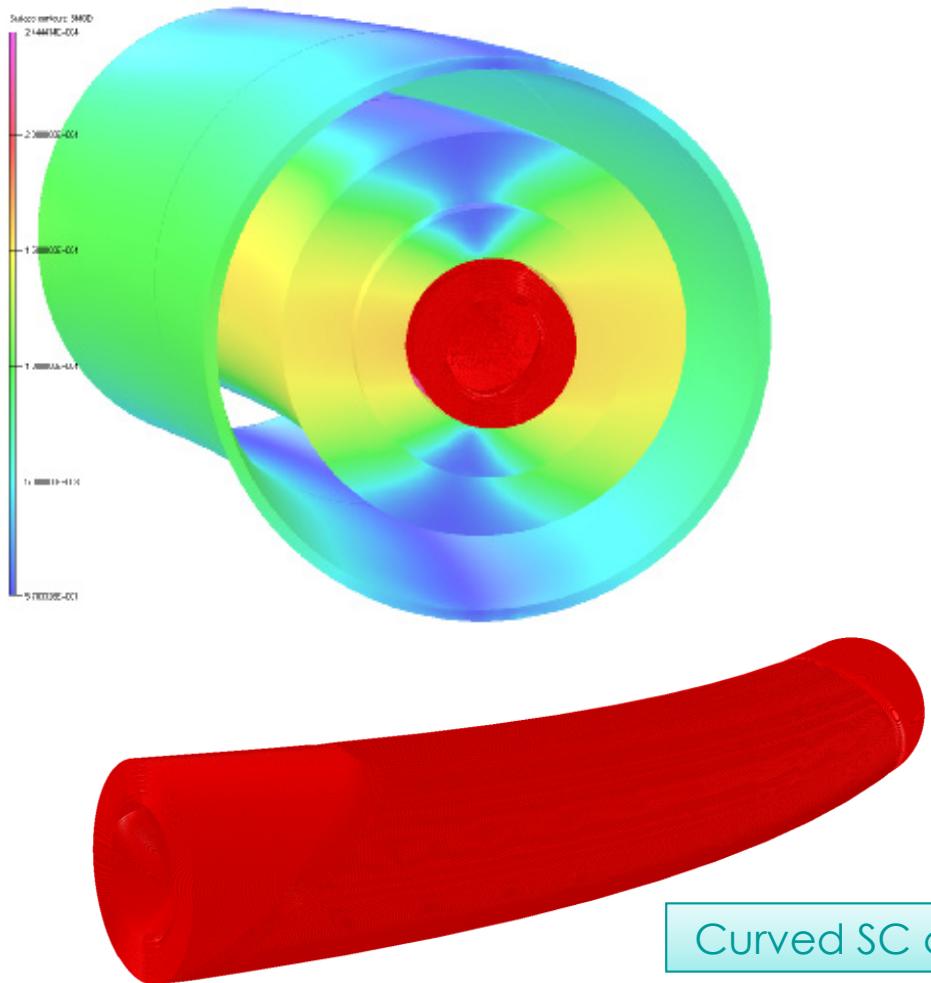
2D field calculation
(BM02-BM05)



3D field calculation with Opera-3d



SC coils were precisely modelled

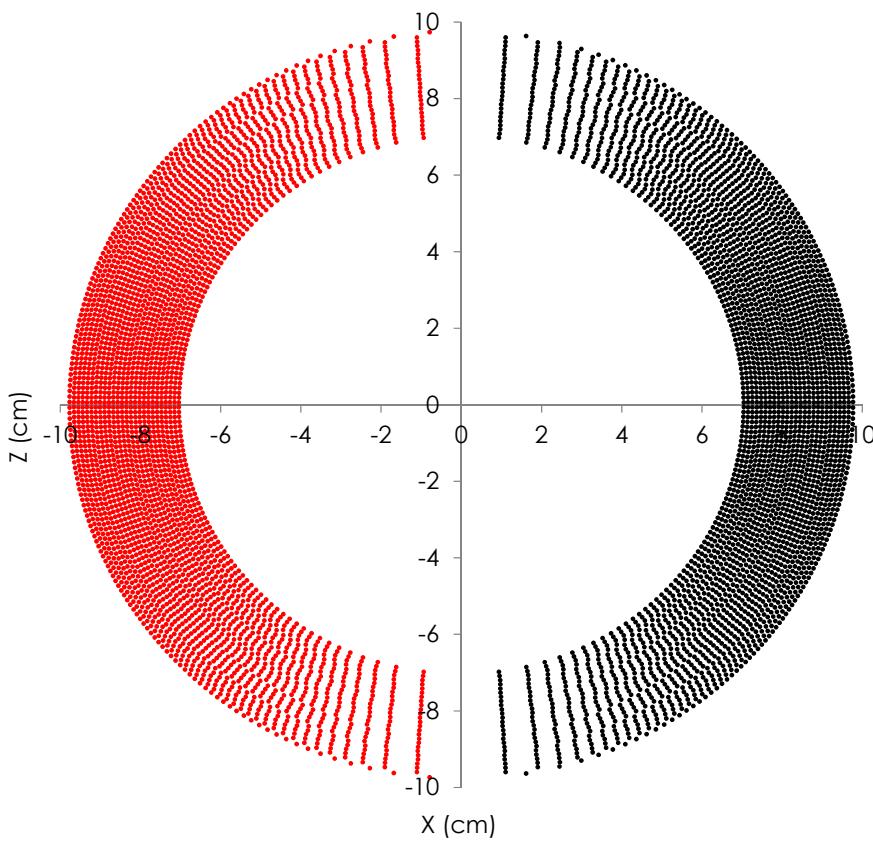


$|\Delta B_{ZL}/B_{ZL}| < 4 \times 10^{-4}$

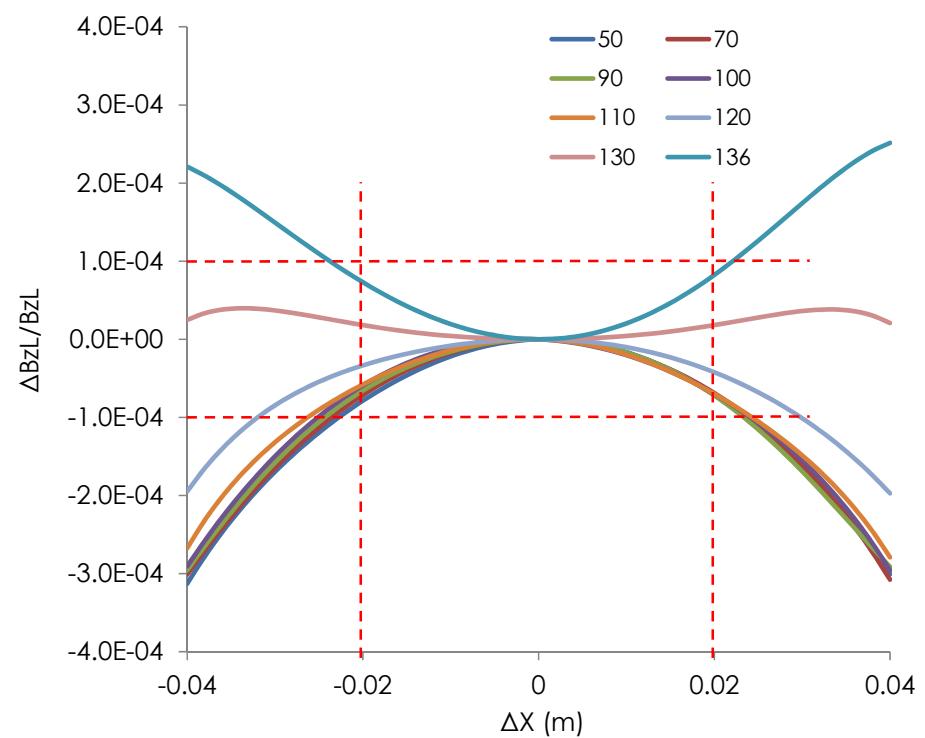
30

Corrections with the outermost layer

Coil positions of the outermost layer were modified to cancel out the measured multi-pole components



Corrected uniformity

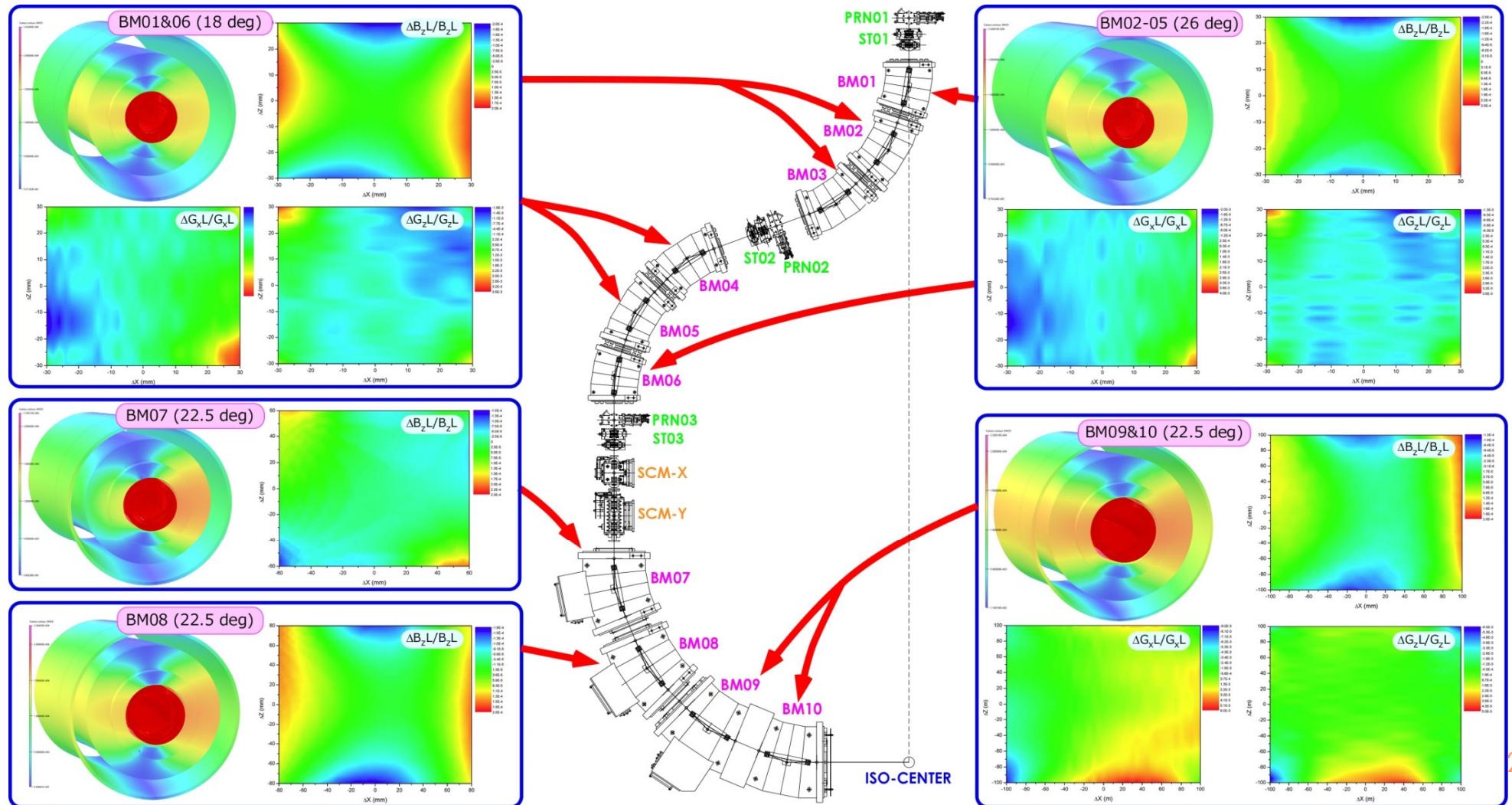


$|\Delta BL/BL| < 1 \times 10^{-4}!$

Design of SC magnets



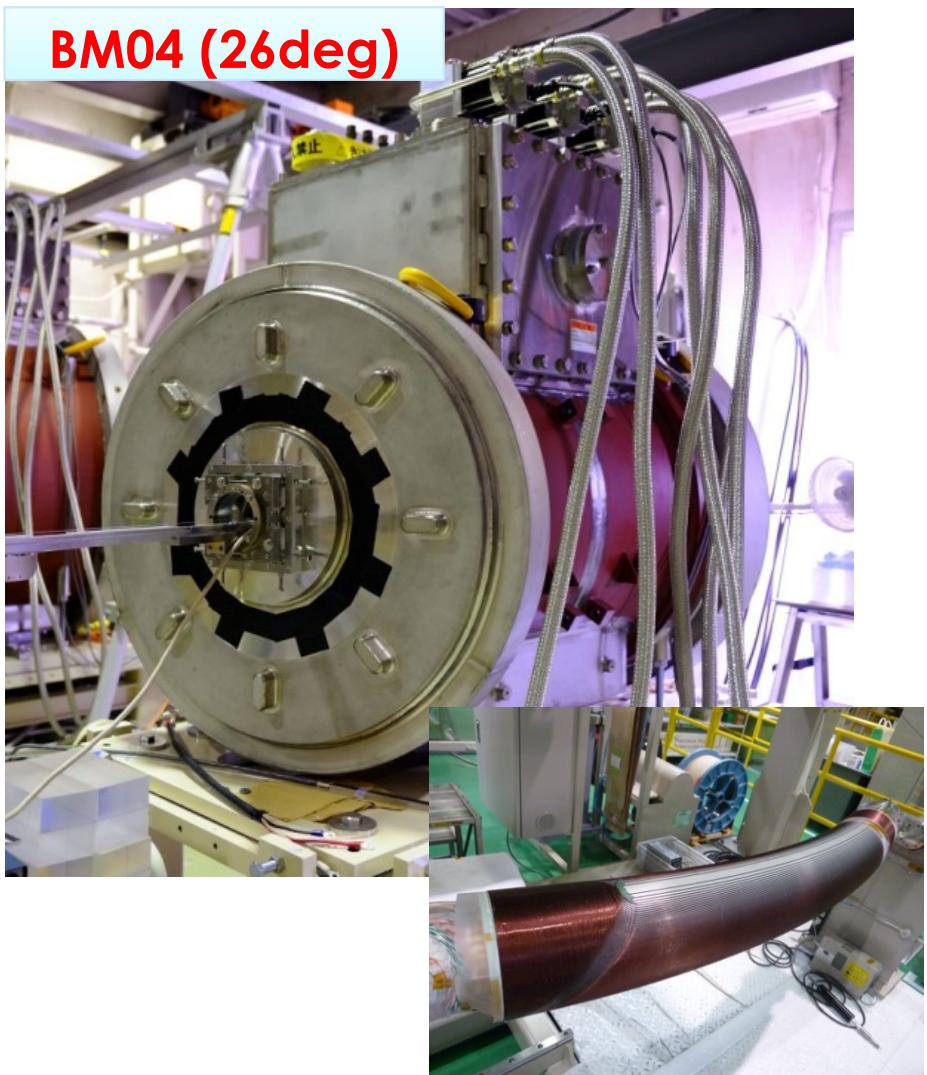
All the SC magnets were designed by using a 3D magnetic field solver



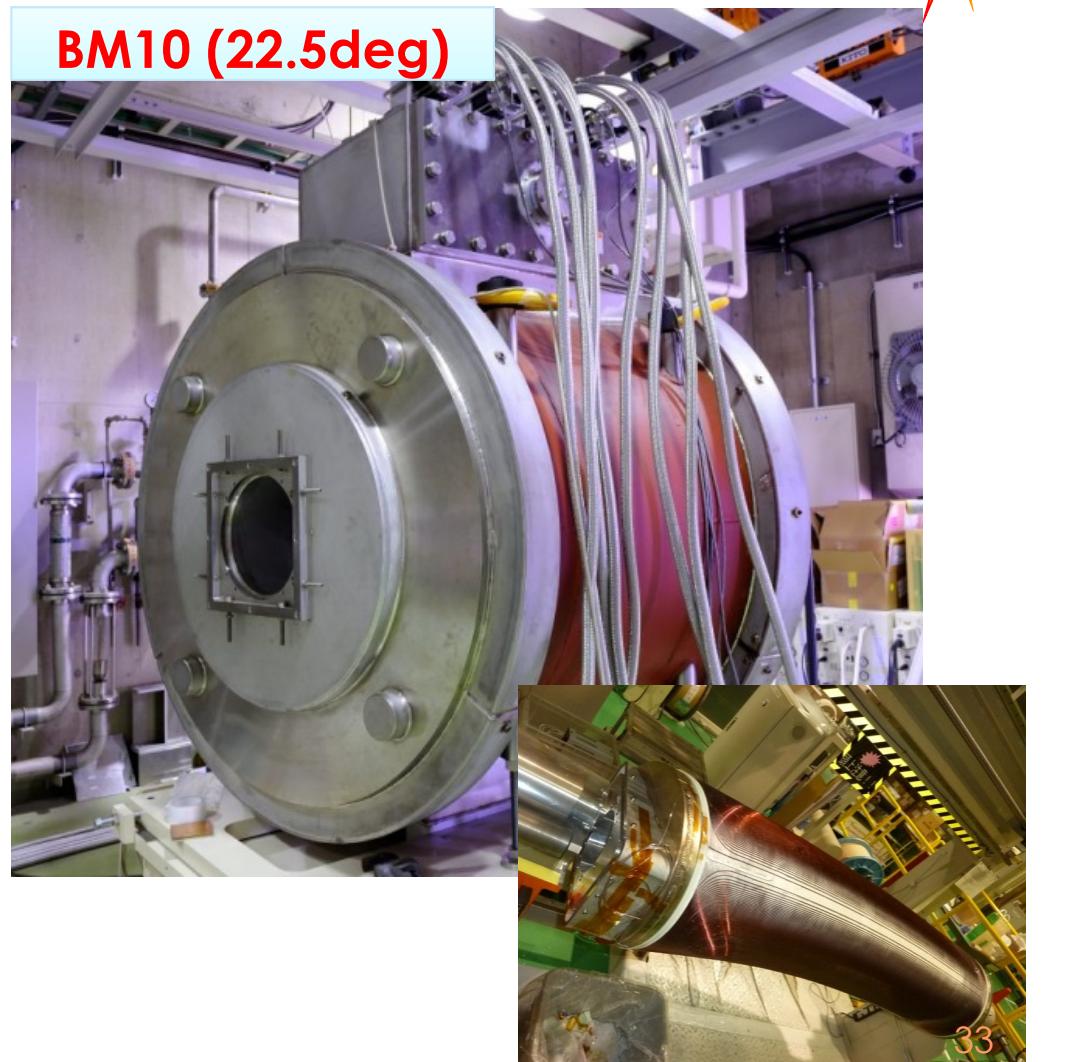
Construction of SC magnets



BM04 (26deg)



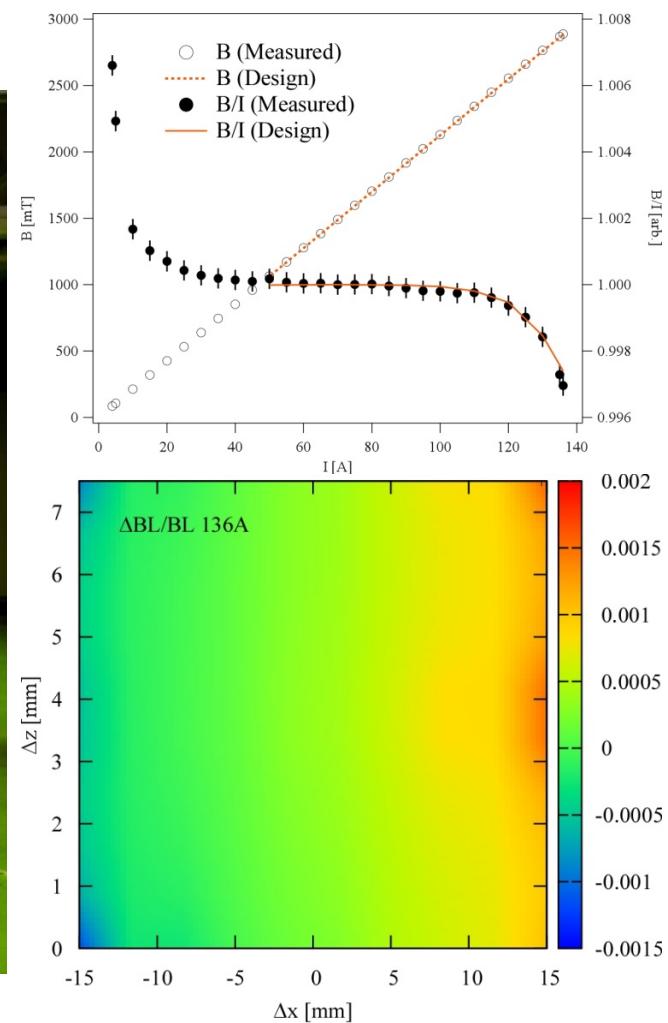
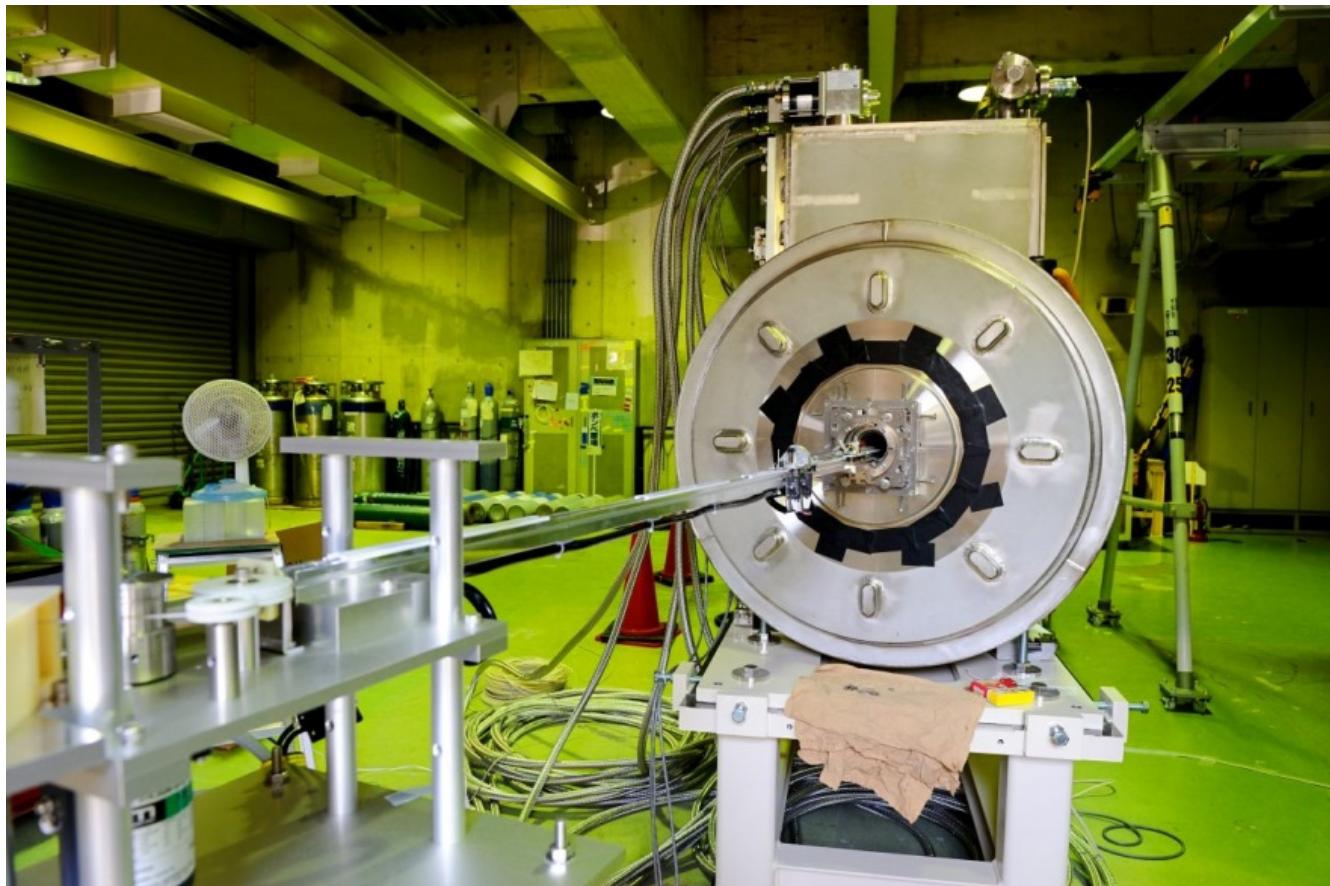
BM10 (22.5deg)



Field measurements



- Magnetic field measurements were performed
 - to verify the SC magnet design





Construction of the gantry structure

Construction of structure



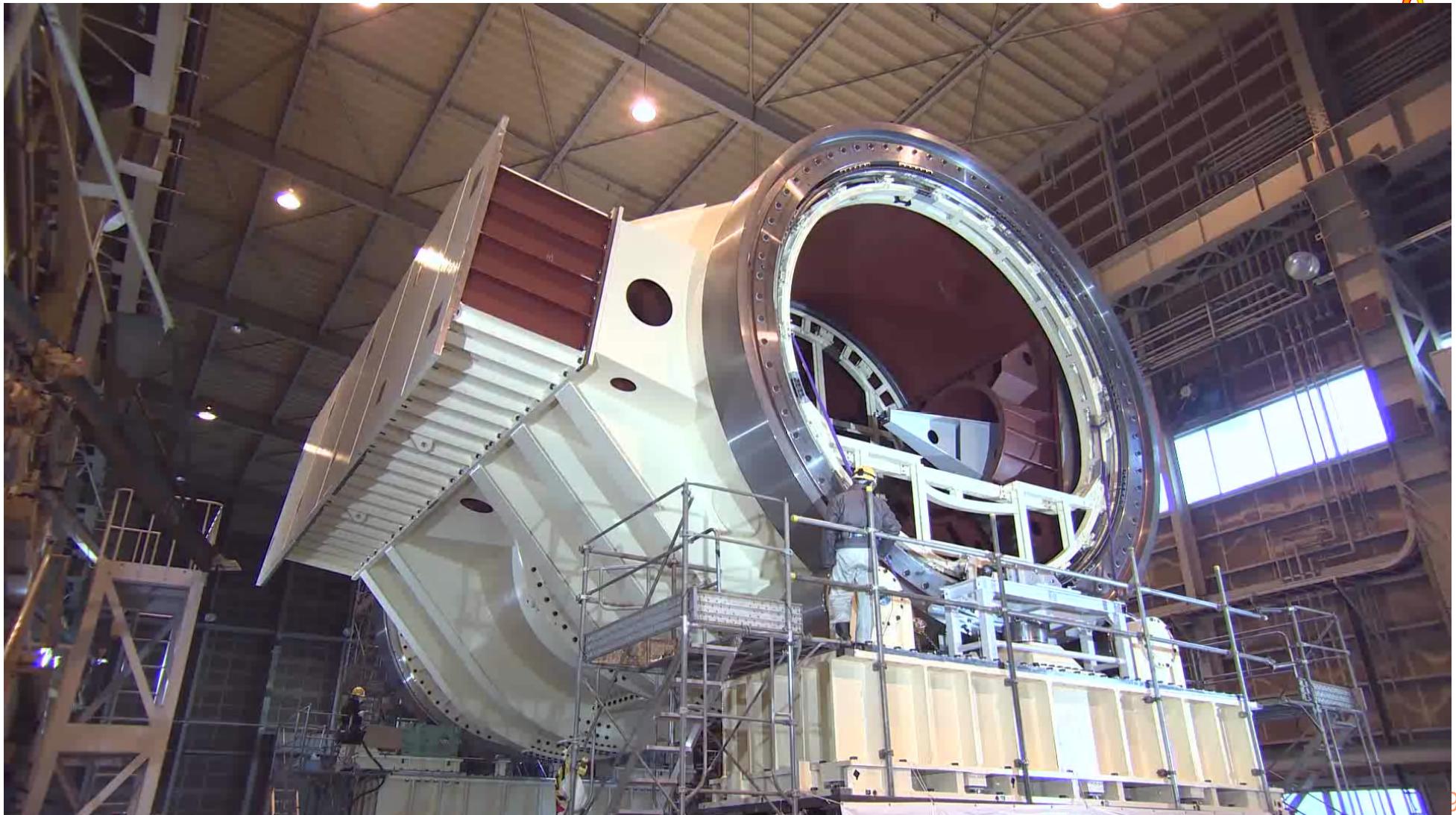
Assembling at Toshiba



Assembling at Toshiba



Rotation tests at Toshiba



Transportation to NIRS



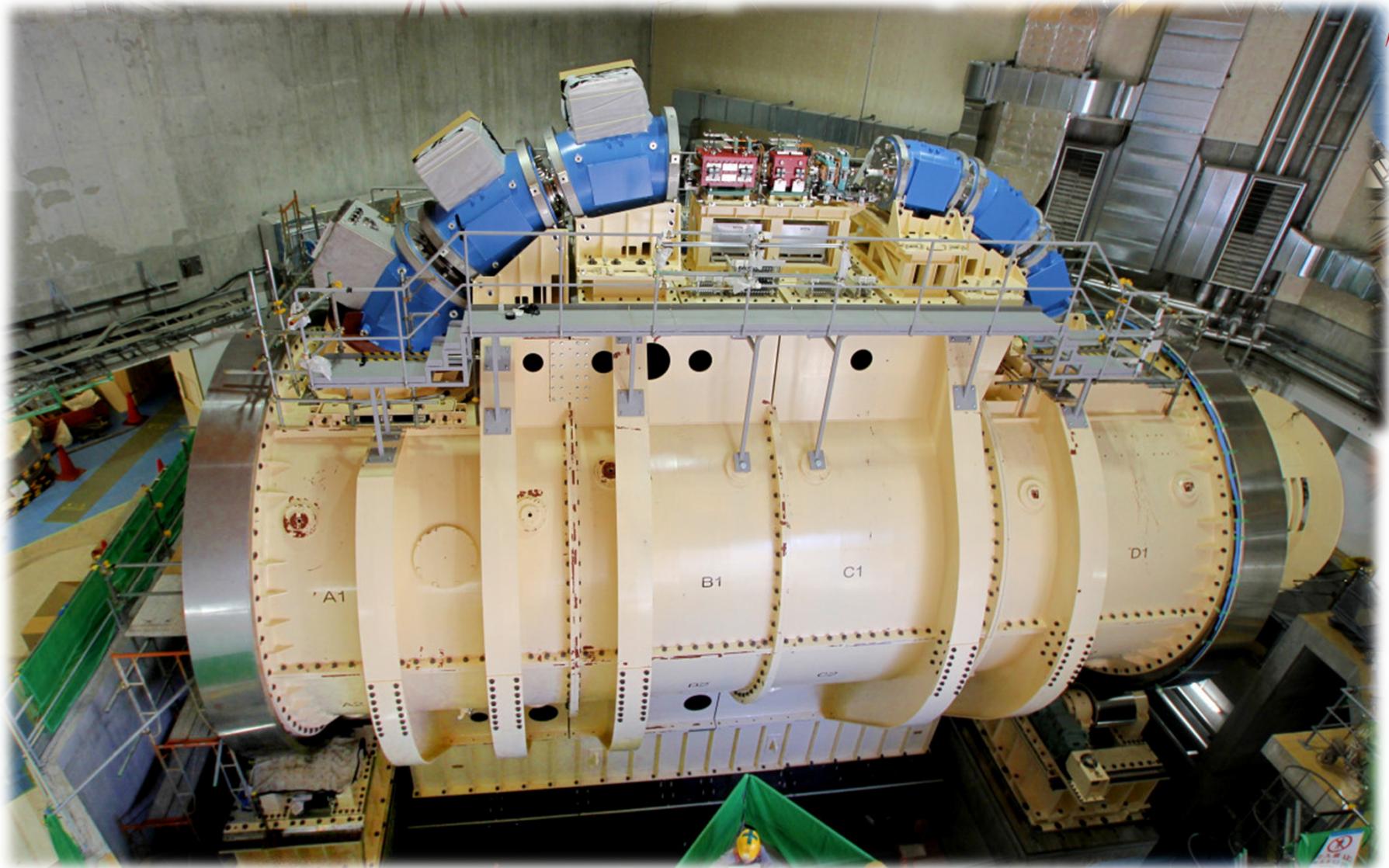
Installation to the gantry room



Reassembling at NIRS



Reassembling at NIRS



Treatment-room design



- The treatment room for the gantry is designed, based on the existing room E & F



Treatment-room design



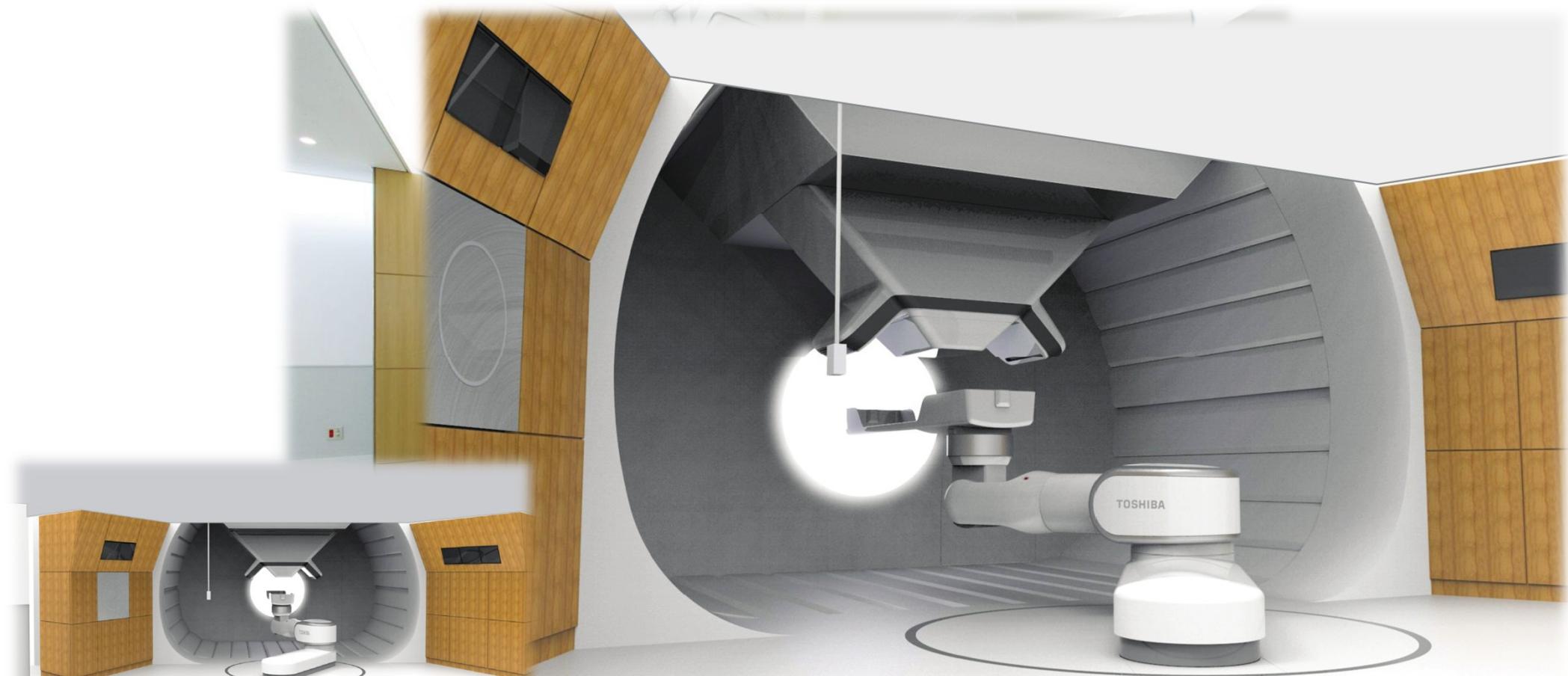
- The treatment room for the gantry is designed, based on the existing room E & F



Treatment-room design



- The treatment room for the gantry is designed, based on the existing room E & F





■ Design of the superconducting rotating-gantry

- **Compact (~proton gantries)**
- **Construction will be completed by the end of this month**

■ Future plan

- **Commissioning will be made from this October**
- **Treatment will be made in 2016**



Collaborators



- K. Noda, T. Shirai, T. Fujita, T. Furukawa,
K. Mizushima, Y. Hara, Y. Saraya, R. Tansho,
S. Matsuba, S. Mori, S. Sato, K. Shoda (NIRS)
- T. Fujimoto, H. Arai (AEC)
- T. Ogitsu (KEK)
- N. Amemiya (Kyoto Univ.)
- Y. Nagamoto, T. Orikasa, S. Takayama,
(Toshiba)

Specifications of SC magnets



Parameters	Symbol	Unit	BM01	BM02	BM03	BM04	BM05	BM06	BM07	BM08	BM09	BM10
Type	—	—	Superconducting sector magnet									
Coil	—	—	Dipole+Quard.						Dipole	Dipole+Quard.		
Bending angle	θ	deg	18		26		18			22.5		
Bending radius	ρ	m			2.3					2.8		
Maximum field	B_{dipole}	T			2.88					2.37		
Maximum field gradient	G_{\max}	T/m			10				—		1.3	
Bore size	D_{bore}	mm			φ60			<input type="checkbox"/> 122	<input type="checkbox"/> 170		<input type="checkbox"/> 206	
Effective radius or area	D_f or A_f	mm			φ40			<input type="checkbox"/> 120	<input type="checkbox"/> 160		<input type="checkbox"/> 200	
Uniformity (dipole)	$\Delta BL/BL$	—					±1×10 ⁻⁴					
Uniformity (quadrupole)	$\Delta GL/GL$	—					±1×10 ⁻³					
Inductance (dipole)	L	H	6.2		9.1		6.2	5.2	8.9		12	
Stored Energy (dipole)	P	kJ	57		84		57	133	225		319	