# Synthesis and Inpainting-Based MR-CT Registration for Image-Guided Thermal Ablation of Liver Tumors

基于图像生成和补全的MR-CT配准用以肝肿瘤热消融手术的影像学导航

Dongming Wei<sup>1,2,4</sup>, Sahar Ahmad<sup>2</sup>, Jiayu Huo<sup>1</sup>, Wen Peng<sup>3</sup>, Yunhao Ge<sup>4</sup>, Zhong Xue<sup>4</sup>, Pew-Thian Yap<sup>2</sup>, Wentao Li<sup>5</sup>, Dinggang Shen<sup>2(⋈)</sup>, and Qian Wang<sup>1(⋈)</sup>

<sup>1</sup> Institute for Medical Imaging Technology, School of Biomedical Engineering, Shanghai Jiao Tong University, Shanghai 200030, China

wang.qian@sjtu.edu.cn

<sup>2</sup> Department of Radiology and Biomedical Research Imaging Center (BRIC), University of North Carolina at Chapel Hill, Chapel Hill, NC 27599, USA

 ${\tt dgshen@med.unc.edu}$ 

- <sup>3</sup> North China Electric Power University, Beijing, China
- <sup>4</sup> Shanghai United Imaging Intelligence Co., Ltd., Shanghai, China
  - <sup>5</sup> Shanghai Cancer Center, Fudan University, Shanghai, China

### BackGround and Contribution

#### □热消融:

- 升高了肿瘤局部区域的温度(55°-65°摄氏度),导致不可逆的细胞损伤,最终导致肿瘤细胞凋亡和凝固性坏死
- 因此, 准确定位肿瘤区域至关重要的
- 在热消融过程中,CT成像通常用于<mark>指导介入过程</mark>,其中术前CT (pCT)用于规划,术中 捕获术中CT (iCT)

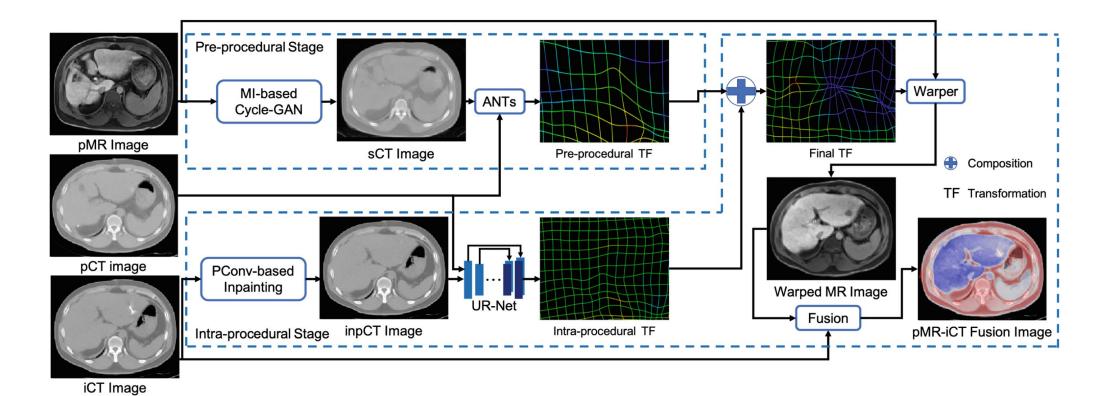
### □存在的问题:

- CT在组织对比度(如动脉)方面相对较差,而且容易受到手术过程中探头引入的<mark>伪影</mark>的影响。
- 高分辨率pCT和程序前MR (pMR)图像通常在规划期间进行对齐,然后在iCT图像上进行配准,可以更精确地指导探测器定位到所需的ROI
- 这种定位的准确性和速度都很重要,因为它可以弥补因患者定位和呼吸运动而造成的不延迟的变形

### BackGround and Contribution

- 大多数配准方法:
  - 没有实时性,只能在准备阶段
  - 没有对手术中,手术器材伪影进行修复
- 本文方案(两阶段):
  - 1. 手术前: MI+CycleGan从pMR图像生成sCT,将交叉模态配准转化为单模态配准问题,将pMR和pCT配准。
  - 2. 手术中: 使用无监督配准网络(URNet), 将inpainted iCT (inpCT)图像与pCT图像快速进行可变形配准。

### Method



ANTs(Advanced Normalized Tools) 是一种传统的精确配准方案

三部分网络: MI-based Cycle-GAN for Synthesis

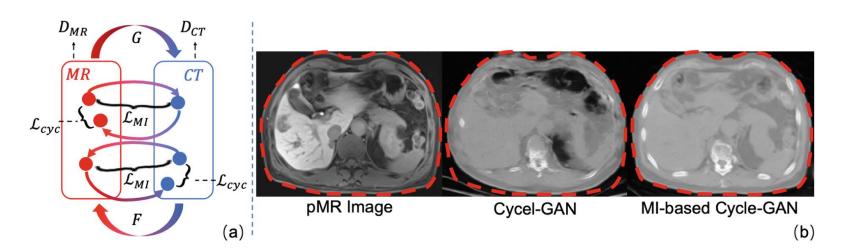
Partial convolution (Pconv-based) inpainting

**UR-Net** 

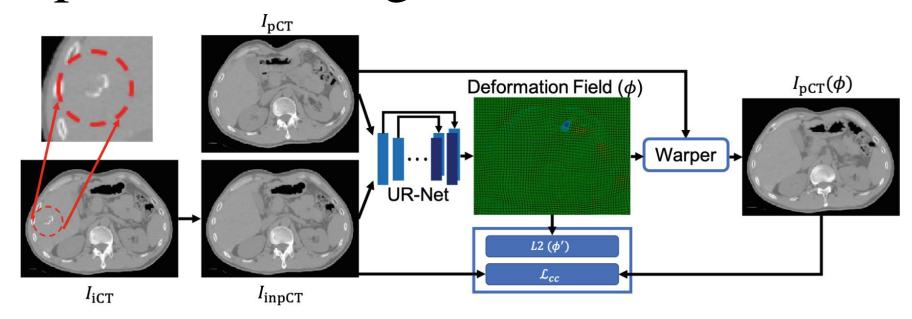
# Cycle-GAN with mutual information constraint

- 跨模态配准:模态间存在很多差异,一个主流方案是转化为单模态问题
- 直接采用CycleGAN会引入边缘的漂移,因此引入互信息约束

$$\mathcal{L}_{\text{MI}} = \sum \sum p(x, y) \log \frac{p(x, y)}{p(x)p(y)}$$



### Intra-procedural Registration



• 实际上就是VoxelMorph的结构

$$\mathcal{L} = -\mathrm{S}(I_{\mathrm{inpCT}}, I_{\mathrm{pCT}}(\phi)) + \mathrm{Reg}(\phi),$$

- 部分卷积网络:
  - 给定一个覆盖探测器及其工件的粗糙掩模(例如,一个边界框或一个多边形), inpainting网络可以重建底层组织并逐层更新掩模,直到掩模缩小
  - 将3D unet中的卷积模块改成Partial Conv

### Partial Convolutional

卷积模块加入一个Mask, 标记有效区域

$$x' = \begin{cases} \mathbf{W}^T (\mathbf{X} \odot \mathbf{M}) \frac{\text{sum}(\mathbf{1})}{\text{sum}(\mathbf{M})} + b, & \text{if sum}(\mathbf{M}) > 0 \\ 0, & \text{otherwise} \end{cases}$$

每一次卷积之后,更新mask。只有这个位置在卷积时存在1个有效 区域的输出,这个位置的mask就更新为1

$$m' = \begin{cases} 1, & \text{if } \text{sum}(\mathbf{M}) > 0 \\ 0, & \text{otherwise} \end{cases}$$

损失函数两个区域分别计算

$$\mathcal{L}_{hole} = \frac{1}{N_{\mathbf{I}_{gt}}} \| (1 - M) \odot (\mathbf{I}_{out} - \mathbf{I}_{gt}) \|_1, \mathcal{L}_{valid} = \frac{1}{N_{\mathbf{I}_{gt}}} \| M \odot (\mathbf{I}_{out} - \mathbf{I}_{gt}) \|_1$$

"感知损失", $\varPsi_p^{\mathbf{I}_*}$  is the activation map of the p-th selected layer given original input

"风格损失", Kp is the normalization fact  $1/C_p H_p W_p$ 

$$\mathcal{L}_{perceptual} = \sum_{p=0}^{P-1} \frac{\|\boldsymbol{\varPsi}_{p}^{\mathbf{I}_{out}} - \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}}\|_{1}}{N_{\boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}}}} + \sum_{p=0}^{P-1} \frac{\|\boldsymbol{\varPsi}_{p}^{\mathbf{I}_{comp}} - \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}}\|_{1}}{N_{\boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}}}}$$

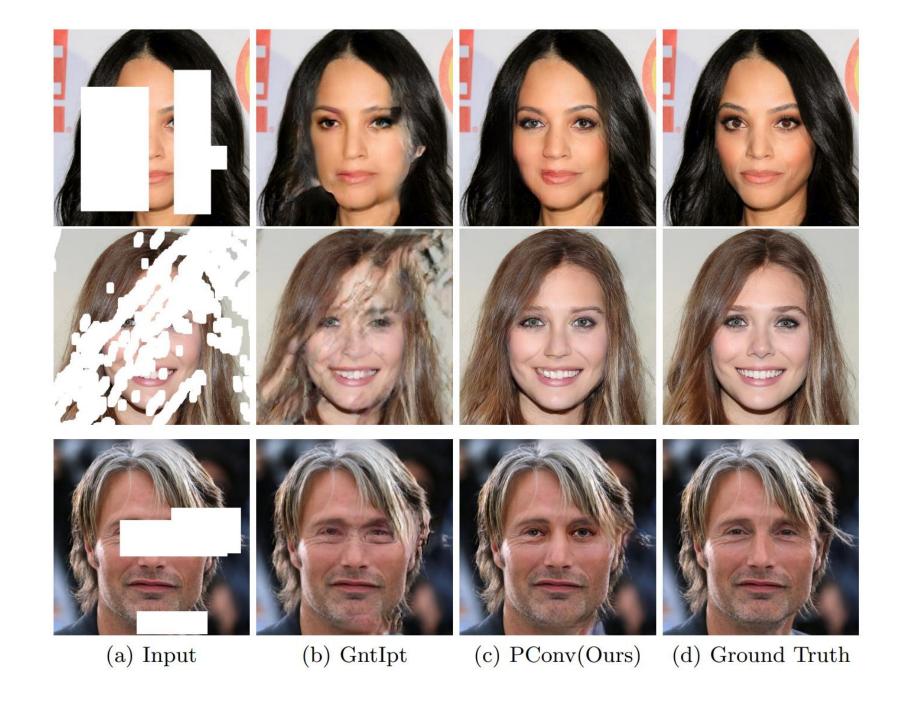
$$\mathcal{L}_{style_{out}} = \sum_{p=0}^{P-1} \frac{1}{C_{p}C_{p}} \left| \left| K_{p} \left( \left( \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{out}} \right)^{\mathsf{T}} \left( \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{out}} \right) - \left( \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}} \right)^{\mathsf{T}} \left( \boldsymbol{\varPsi}_{p}^{\mathbf{I}_{gt}} \right) \right) \right| \right|_{1}$$

$$\mathcal{L}_{style_{comp}} = \sum_{p=0}^{P-1} \frac{1}{C_p C_p} \left| \left| K_p \left( \left( \Psi_p^{\mathbf{I}_{comp}} \right)^{\mathsf{T}} \left( \Psi_p^{\mathbf{I}_{comp}} \right) - \left( \Psi_p^{\mathbf{I}_{gt}} \right)^{\mathsf{T}} \left( \Psi_p^{\mathbf{I}_{gt}} \right) \right| \right|_1$$

### Partial Convolutional

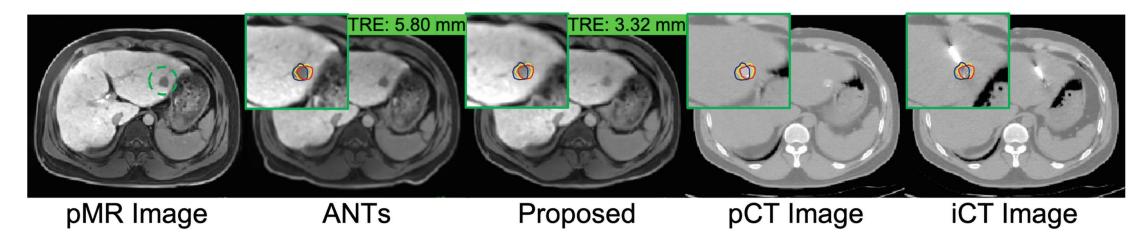
平滑损失,R where R is the region of 1-pixel dilation of the hole 
$$\mathcal{L}_{tv} = \sum_{(i,j) \in R, (i,j+1) \in R} \frac{\|\mathbf{I}_{comp}^{i,j+1} - \mathbf{I}_{comp}^{i,j}\|_1}{N_{\mathbf{I}_{comp}}} + \sum_{(i,j) \in R, (i+1,j) \in R} \frac{\|\mathbf{I}_{comp}^{i+1,j} - \mathbf{I}_{comp}^{i,j}\|_1}{N_{\mathbf{I}_{comp}}}$$

$$\mathcal{L}_{total} = \mathcal{L}_{valid} + 6\mathcal{L}_{hole} + 0.05\mathcal{L}_{perceptual} + 120(\mathcal{L}_{style_{out}} + \mathcal{L}_{style_{comp}}) + 0.1\mathcal{L}_{tv}$$



## Dataset and Pre-processing

- 39例数据 undergoing liver tumor ablation were included in our experiment
- 全部具有pMR, pCT and iCT
- 11例测试, 28例训练
- 256 × 256 × 128 with isotropic voxel distances



**Table 2.** Results of pMR-iCT (rigid and deformable), pMR-pCT (rigid and deformable), and pCT-iCT (deformable only) registration.

		Rigid		Deformable	
		FLIRT	ANTs	ANTs	Proposed
pMR-iCT					
Liver	Dice (%)	$48.44 \pm 40.40$	$85.52 \pm 2.92$	$86.59 \pm 3.30$	$86.96 \pm 3.00$
	TRE (mm)	-	$52.56 \pm 9.85$	$5.18 \pm 2.43$	$4.93 \pm 2.72$
pMR-pCT					
Liver	Dice (%)	$48.07 \pm 40.40$	$87.03 \pm 2.60$	$89.55 \pm 2.04$	$90.59 \pm 1.73$
	TRE (mm)	-	$6.63 \pm 2.73$	$5.59 \pm 2.01$	$4.67 \pm 2.00$
Tumor	Dice (%)	$12.88 \pm 25.76$	$51.10 \pm 17.13$	$55.34 \pm 5.70$	$62.45 \pm 4.66$
	TRE (mm)	-	$6.71 \pm 2.27$	$6.08 \pm 1.40$	$3.89 \pm 0.99$
pCT-iCT					
Liver	Dice (%)	-	-	$87.90 \pm 5.25$	$88.63 \pm 5.53$
	TRE (mm)	-	-	$5.06 \pm 3.29$	$4.37 \pm 3.30$

