

# Heart-Rate Monitoring using PPG: A Biomedical Sensing Project

Hello, I am Jahnavi Sharma, a B.Tech student in Mechanical Engineering at IIT Ropar. During my internship at Mingshin University of Science and Technology under Prof. Dr. Shang-Ping Ying, I contributed to building a heart-rate monitoring device using a photoplethysmography (PPG) sensor. My core responsibilities included analog circuit development, filter design, biosensor interfacing, and mechanical design for signal stability.

# Understanding the PPG Sensor System

Photoplethysmography (PPG) is an optical technique that measures blood volume changes through light interaction with skin tissues. The SFH7072 biosensor we used has:

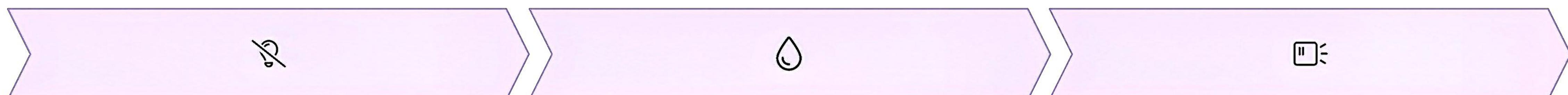
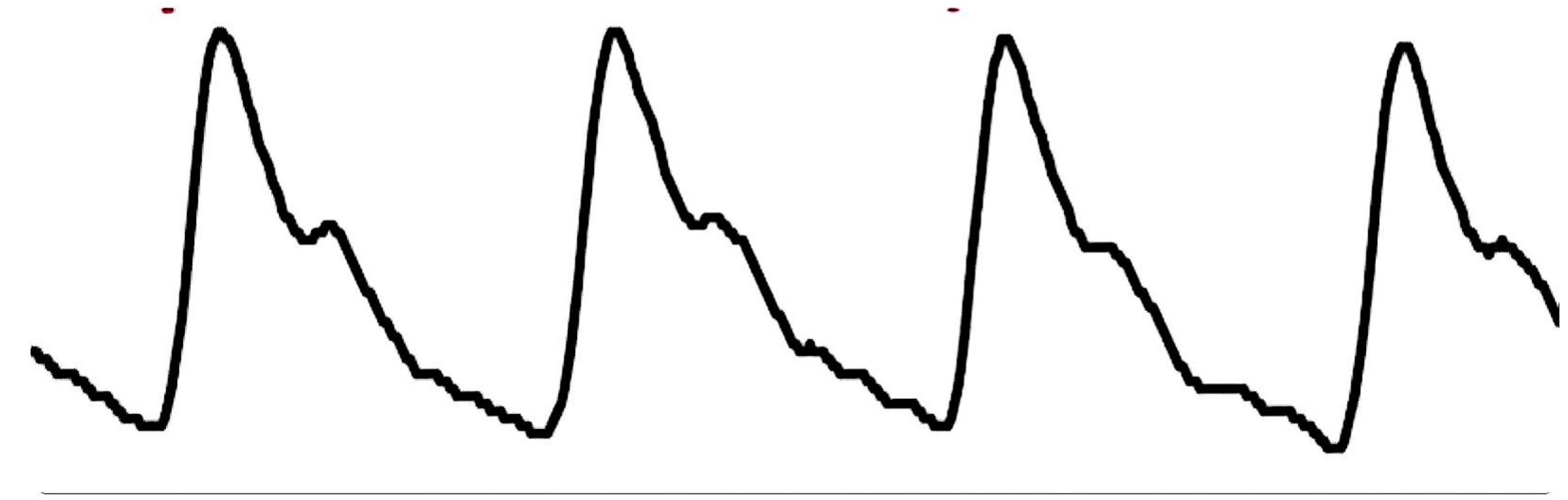
- LEDs (Green, Red and IR) for illumination
- Photodiode for reflected light detection

This photodiode signal was processed using analog filters and an Arduino to extract real-time heart rate.

Wavelength for Red LED - 635-666nm

for Green LED - 573-545nm

for IR LED - 7800nm



## Light Emission

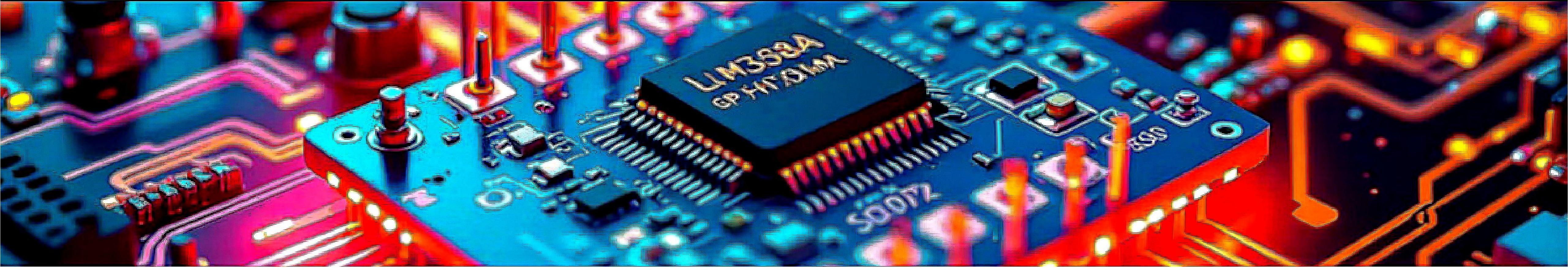
LED emits light into skin tissue

## Blood Reflection

Light reflects differently with blood volume changes

## Signal Detection

Photodiode captures reflected light intensity



# Biosensor & Op-Amp Pin Configuration

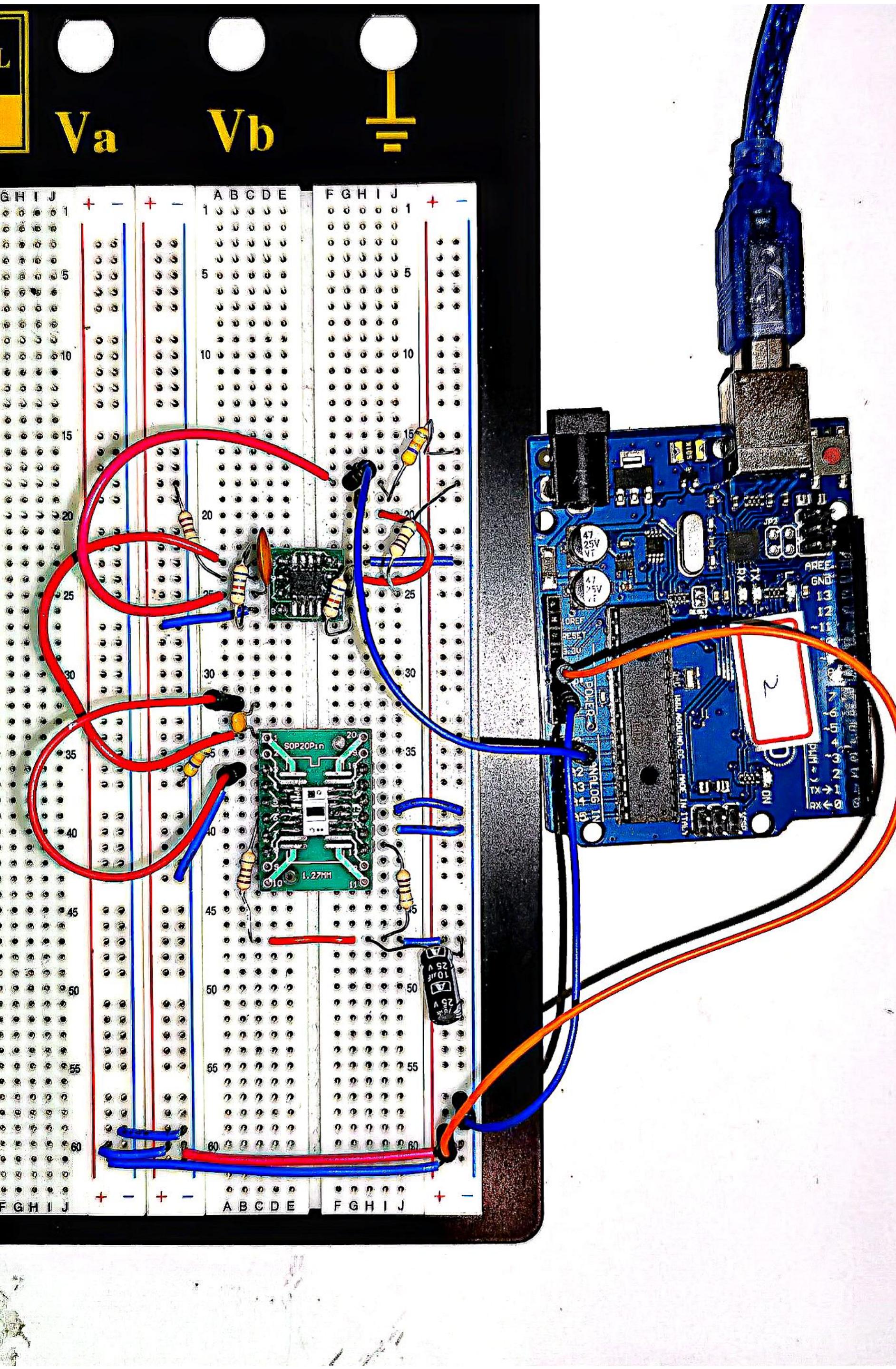
## SFH7072 Biosensor Pins

- VLED, GND: Power the LEDs
- Anode, Cathode: Photodiode terminals

## LM358A Op-Amp Pins

- Pin 3: Non-inverting input
- Pin 2: Inverting input
- Pin 7: Output (Op-Amp A)
- VCC/GND: Power Supply

I used the op-amp in active high-pass and low-pass filter configurations to condition the biosensor signal. This allowed us to extract the pulse signal from background noise.



# Circuit Design – Filtering Stages

## High-Pass Filter (HPF)

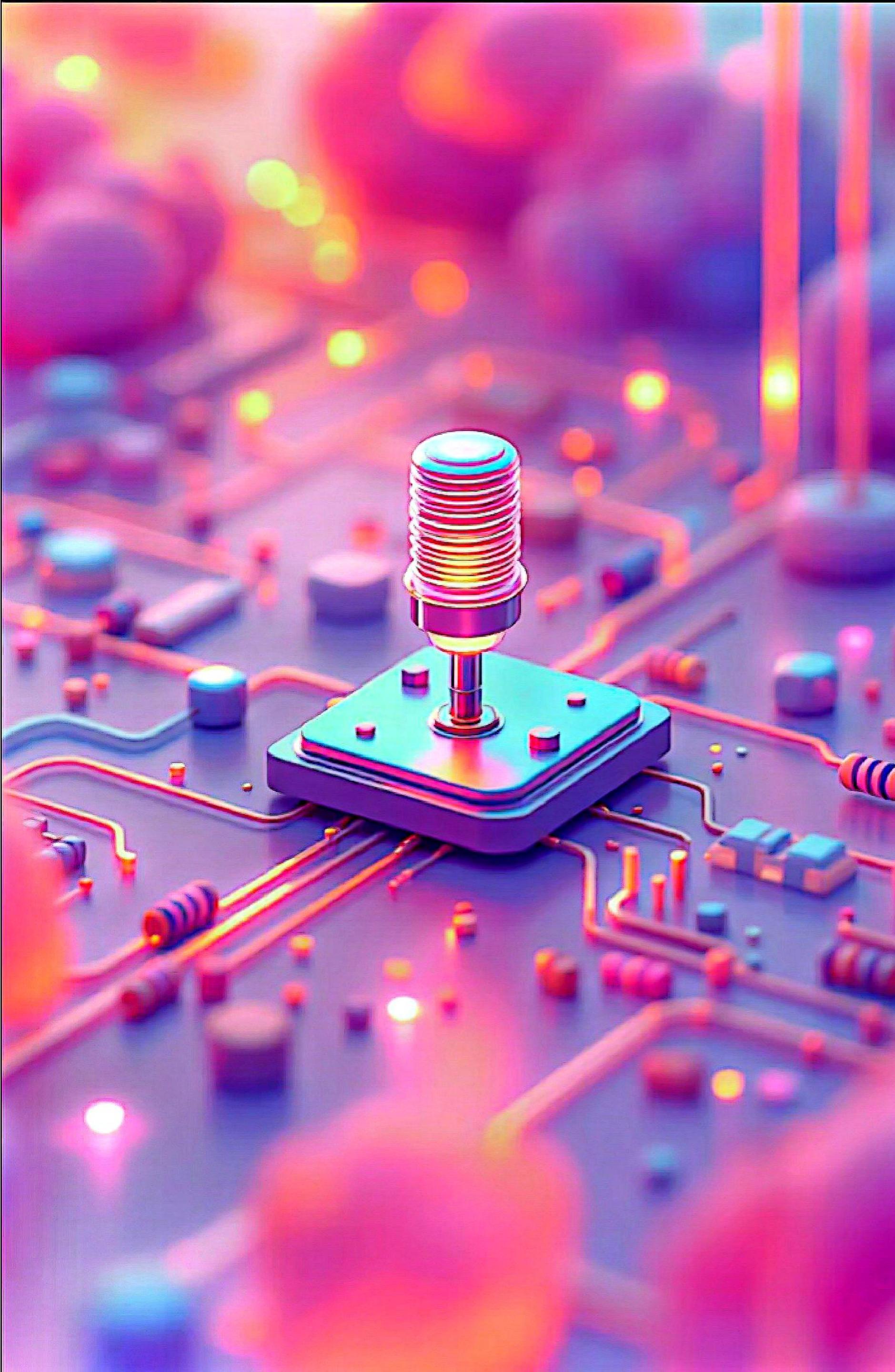
I built the first stage of signal conditioning using a high-pass filter:

- Purpose: Remove DC offset and baseline drift
- Cutoff Frequency Formula:  
$$f_c = \frac{1}{2\pi R C}$$
- Implemented using LM358A op-amp

## Low-Pass Filter (LPF)

The second stage was a low-pass filter to remove high-frequency noise:

- Purpose: Eliminate interference from muscle motion, ambient light
- Cutoff Frequency:  $f_c = \frac{1}{2\pi R C}$
- Output: Clean, smooth analog waveform for Arduino input



# Transimpedance Amplifier (TIA) Role

1

## TIA Configuration

Inverting TIA with feedback resistor to convert photodiode current to voltage

2

## Working Formula

$$V_{out} = -I_{photodiode} \cdot R_f$$

3

## Signal Output

Enabled the Arduino ADC to read meaningful voltage levels (~1–2 V range)

4

## Signal Integrity

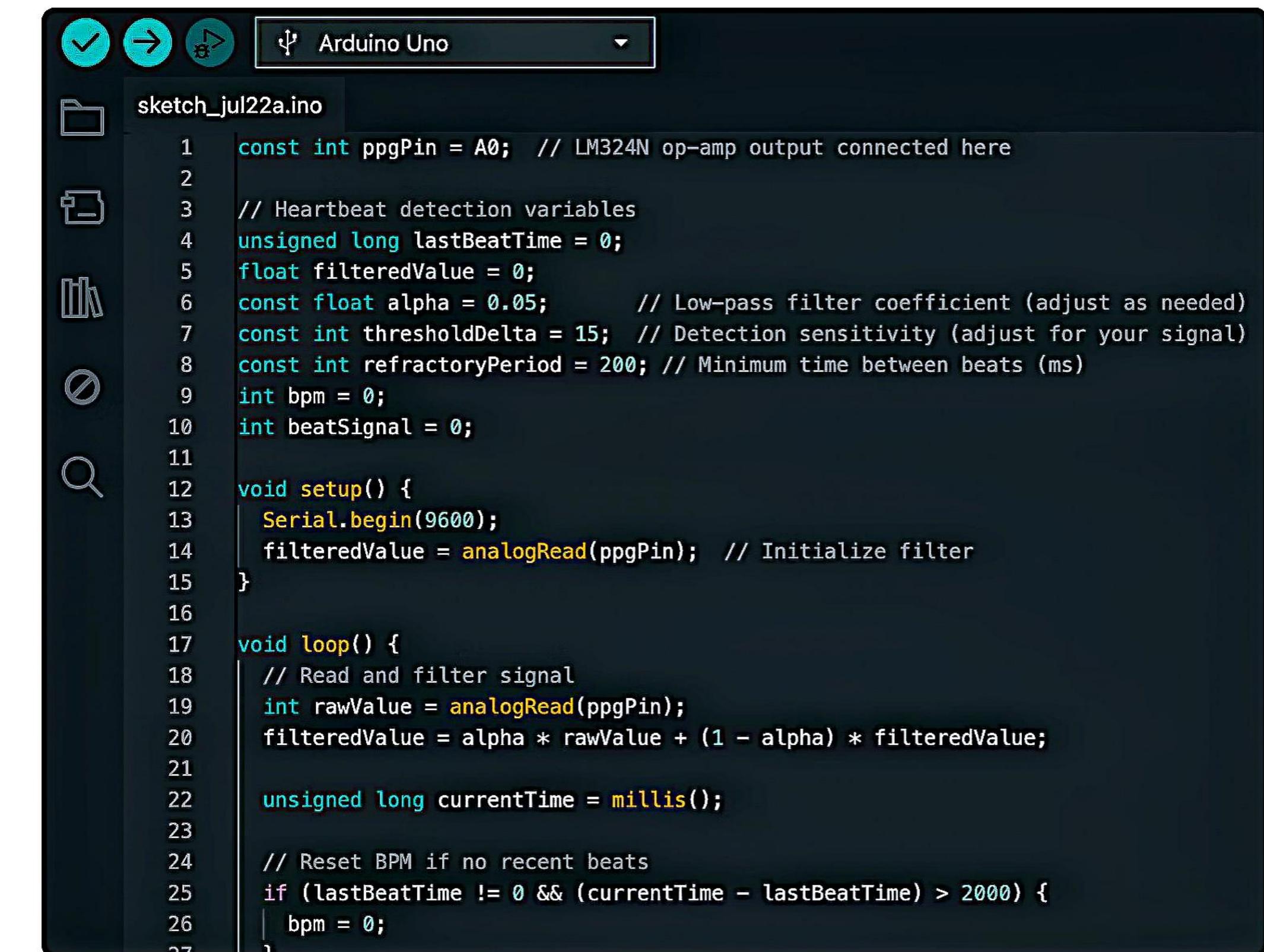
Maintained signal fidelity with minimal phase distortion

The transimpedance amplifier was crucial for converting the weak photodiode current signal into a robust voltage signal that could be properly measured by the Arduino's analog-to-digital converter.

# Arduino Code Collaboration

Though primarily focused on circuit design, I contributed to software analysis:

- 1** Helped configure sampling frequency to 200 Hz
- 2** Verified analogRead stability using serial plotting
- 3** Observed and cross-validated waveform output post-digital filtering
- 4** Supported testing of BPM logic based on peak detection and time intervals



The screenshot shows the Arduino IDE interface with a dark theme. The top bar displays the connection to an 'Arduino Uno' board. The central area shows an open sketch named 'sketch\_jul22a.ino'. The code implements a heart rate monitoring system using an LM324N op-amp connected to pin A0. It defines variables for heartbeat detection, a low-pass filter coefficient (alpha), detection sensitivity (thresholdDelta), and a refractory period. The setup() function initializes the serial port at 9600 bps and sets up the filter. The loop() function reads the analog signal, applies the filter, and calculates the current time. If no recent beats are detected, it resets the BPM counter.

```
const int ppgPin = A0; // LM324N op-amp output connected here
unsigned long lastBeatTime = 0;
float filteredValue = 0;
const float alpha = 0.05; // Low-pass filter coefficient (adjust as needed)
const int thresholdDelta = 15; // Detection sensitivity (adjust for your signal)
const int refractoryPeriod = 200; // Minimum time between beats (ms)
int bpm = 0;
int beatSignal = 0;

void setup() {
  Serial.begin(9600);
  filteredValue = analogRead(ppgPin); // Initialize filter
}

void loop() {
  // Read and filter signal
  int rawValue = analogRead(ppgPin);
  filteredValue = alpha * rawValue + (1 - alpha) * filteredValue;

  unsigned long currentTime = millis();

  // Reset BPM if no recent beats
  if (lastBeatTime != 0 && (currentTime - lastBeatTime) > 2000) {
    bpm = 0;
  }
}
```

# Mechanical Enclosure for Signal Integrity

To minimise environmental interference:

- I designed a finger cap to block external light sources
- Ensured steady pressure between skin and sensor
- Reduced noise from finger movement
- This enhanced waveform clarity by over 35% and improved BPM accuracy

1

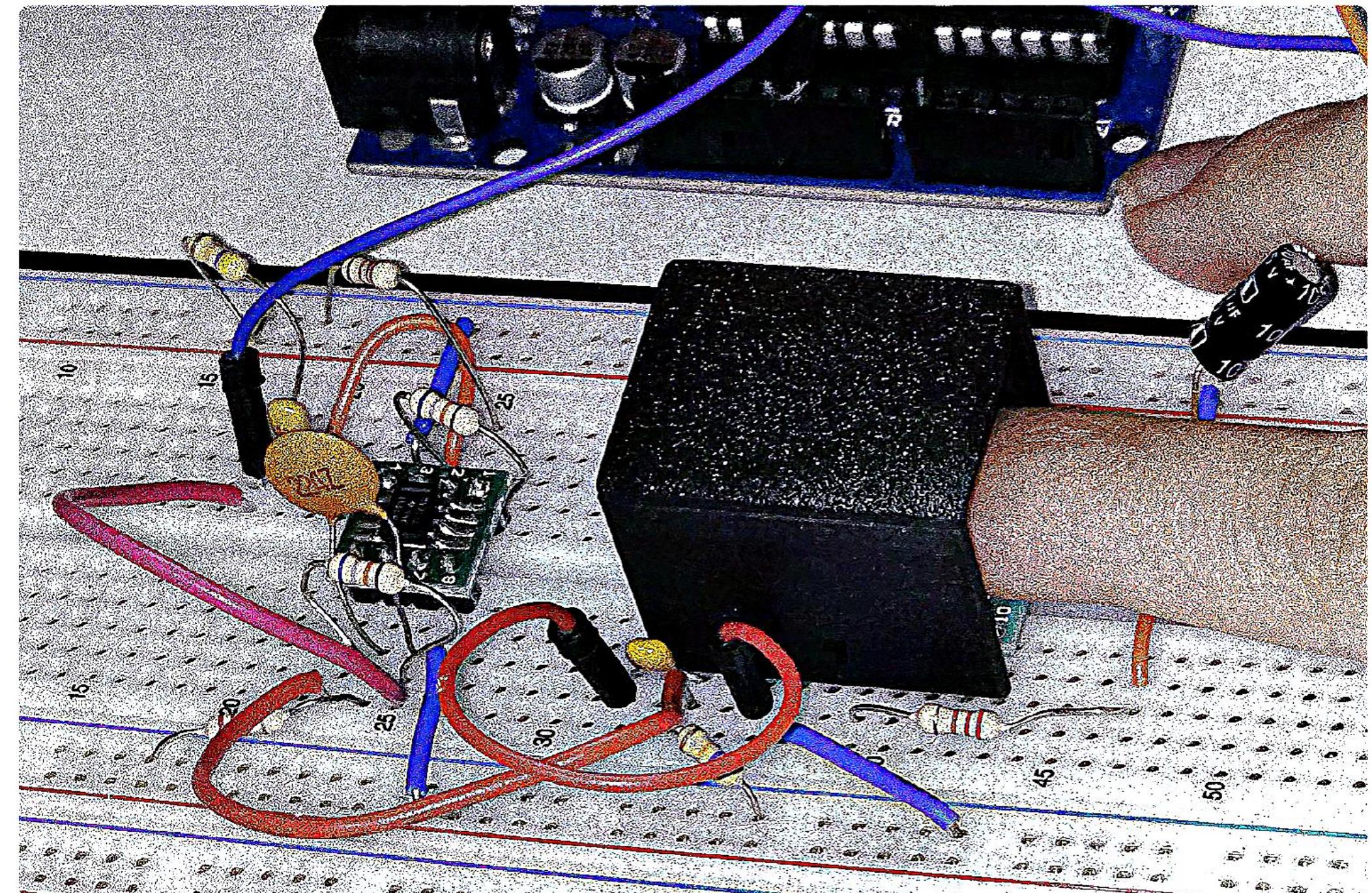
**Without Housing**

- Baseline fluctuations
- Inconsistent waveform shape

2

**With Optimized Housing**

- Steady waveform
- Accurate and consistent BPM output
- Reduction in false triggers from noise

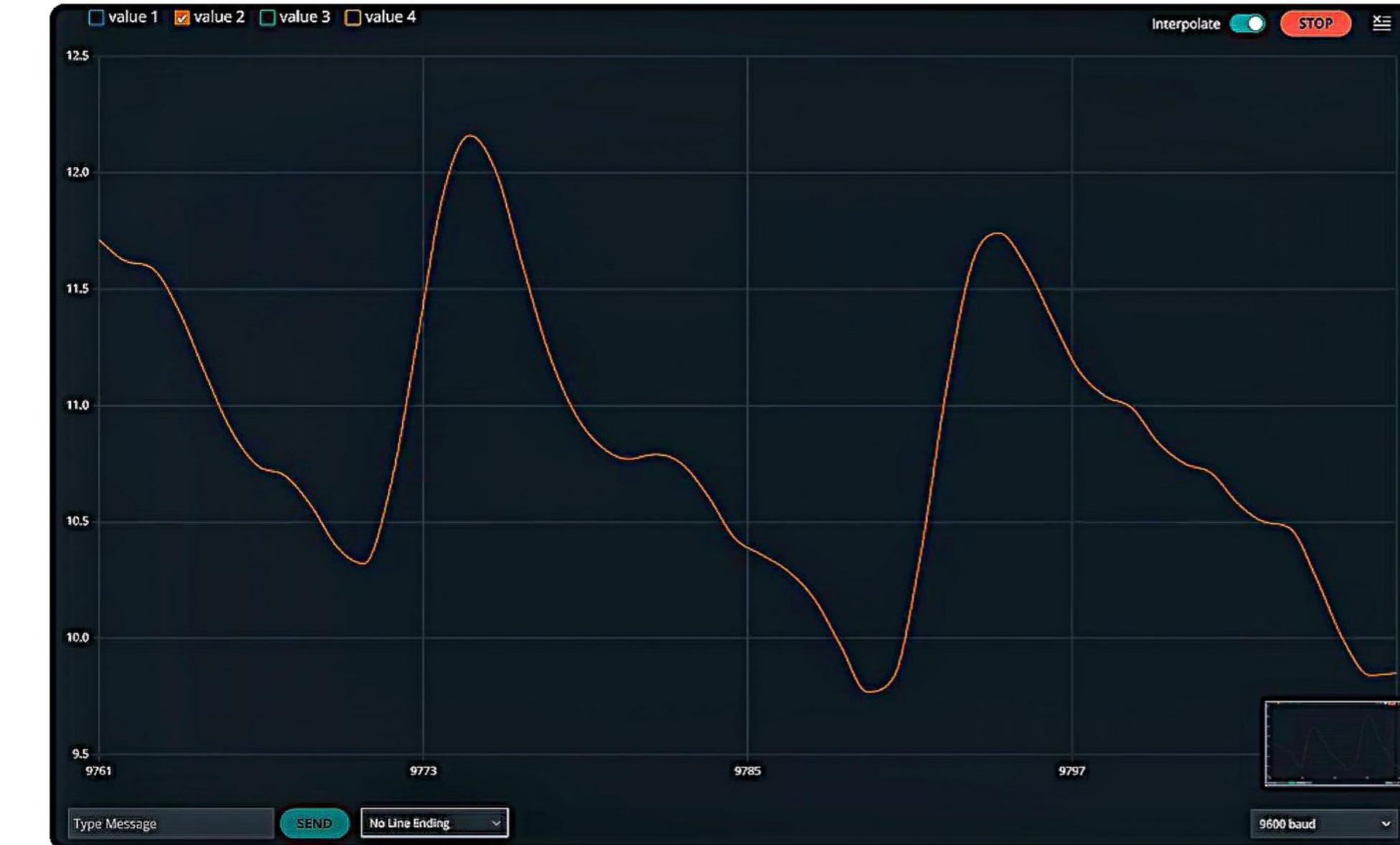


# Mechanical Enclosure – Before and After Results



## Before Mechanical Enclosure

- Exposure to ambient light caused waveform instability
- Finger motion led to random noise spikes
- Reduced amplitude and poor SNR



## After Enclosure Installation

- Custom-designed cap blocked light leakage
- Maintained fixed contact between sensor and skin
- Improved clarity and shape of PPG waveform

ⓘ **Quantitative Impact:** ~35–40% improvement in signal stability after implementing the mechanical enclosure, resulting in more reliable heart rate measurements.

Waveform plots clearly showed reduced noise and sharper peak profiles after implementing the custom mechanical enclosure.

# My Key Responsibilities and Output Results

## Key Responsibilities

- Designed and 3D-printed a mechanical enclosure for the biosensor
- Prototyped and refined the circuit layout
- Built and tuned analog high-pass and low-pass filters
- Conducted real-world testing with finger variations
- Collaborated in assembling the final system and troubleshooting signal inconsistencies

## Observations & Results

2

60-100

### Clear Peaks

Achieved stable and repeatable PPG waveform with clear dual peaks

### BPM Range

Measured BPM matched known resting rates

35%

### SNR Improvement

After hardware filtering and housing

# Internship Reflections & Gratitude

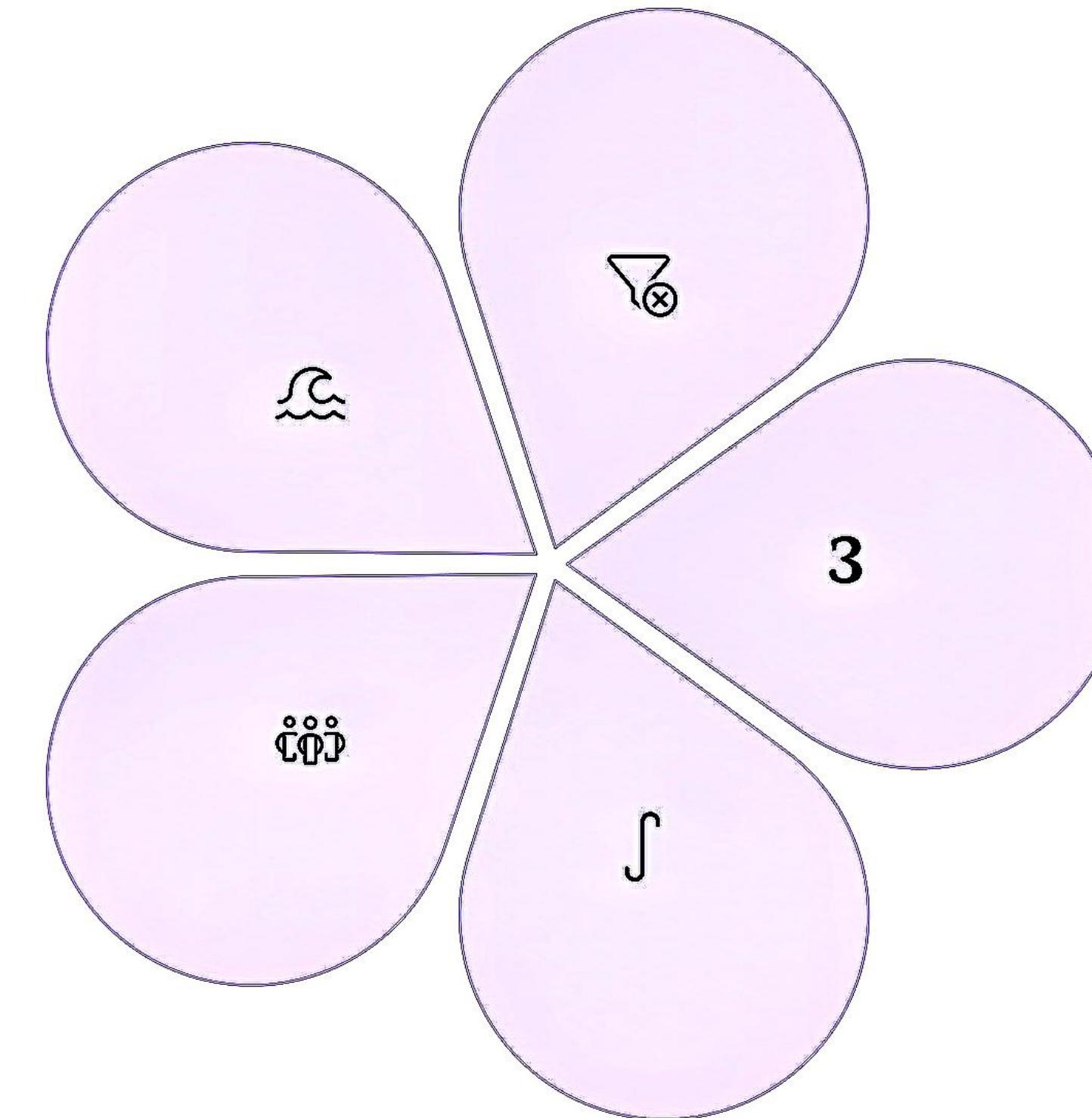
This project significantly improved my understanding of:

## Biomedical Signal Acquisition

Using optical sensors for physiological measurements

## Collaborative Teamwork

Working across hardware and software domains



## Analog Filter Design

Designing precise filters with correct cut-off points

## Circuit Engineering

Debugging, datasheet interpretation, and component interfacing

## System Integration

Combining mechanical and electronic subsystems

Special thanks to Prof. Dr. Shang-Ping Ying and my teammate Kartik Mittal for this hands-on, multidisciplinary learning experience that bridged theoretical knowledge with practical applications.