

Project Proposal

Segmentation in Medical Imaging

Zhaotian Fang (z23fang)

Zhaotian Fang (z23fang)

Zhaotian Fang (z23fang)

October 25, 2019

CS221

Autumn 2019

Stanford University

1 Introduction

In recent years, there has been renewed interest in accurate segmentation of magnetic resonance (MR) images, especially for the human brain. In this task, there are two focus areas: neuroanatomy segmentation on the whole brain as well as anomaly detection and segmentation on the lesion or tumor areas. The neuroanatomy segmentation forms the foundation for volume and shapes analyses to track the progression of diseases over time. Moreover, it provides labelling of brain structures such as the white matter, cortex, hippocampus, etc. to help neuroscience studies. The brain MR images are often used for pathological diagnosis. The accurate detection and segmentation of brain lesions or tumors are even more critical.

2 Related Work

Since manual segmentation of brain neuroanatomy and lesions is time-consuming, there has been a plethora of efforts in automating and accelerating the process. In terms of unsupervised approaches for brain neuroanatomy segmentation, the most commonly used is a software tool named FreeSurfer [1]. There has been an abundance of follow-up research on multi-atlas registration and label fusion (MALF) (citation here). However, these techniques are computationally intensive, taking several hours to produce a single segmentation result. As for brain lesion segmentation, a MATLAB toolbox named Lesion Segmentation Tool (LST) is usually used to identify lesion areas. As a post-processing step, the resulting lesion segmentations are then manually adjusted by radiologists for better precision.

In attempts to improve on the efficiency of brain anatomy segmentation and lesion segmentation, supervised Convolutional Neural Network (CNN) based approaches have been emerging over the past few years. However, these methods are faces two main constraints on performance. First, these supervised models require an extensive amount of high-quality segmentation labels. These labels are usually created manually and thus hard to obtain. Secondly, these models primarily operate on similar applications base on the dataset they were trained on. Due to the high cost associated with label acquisition in addition to hardware limitations, high quality MRI datasets appropriate for training neural networks are limited. As a result, supervised approaches like CNNs struggle with generalization. Therefore, there is a need to find a generalizable model to efficiently segment the brain MR images in an unsupervised manner.

In the medical field, there have been a few attempts to use deep learning with the object to achieve unsupervised segmentation. Stacked denoising autoencoders were used as a pre-training step before supervised learning. (Citations) Generative models such as the AnoGAN framework and Variational Autoencoders were deployed to learn healthy brain images, assuming that when fed with brain images with anomalies, the network will be able to classify the image as abnormal. An effort was made to combine the above-mentioned frameworks into what is called AnoVAEGAN to segment brain lesions in an unsupervised way. However, these approaches are still rely on large sets of high-quality and healthy brain images to learn effectively.

3 Method

Lately, in the computer vision field, a novel method was proposed by Ji Xu et al. to use invariant information clustering (IIC) for unsupervised image classification and segmentation. This method uses a clustering technique where it maximizes the mutual information between the class assignments of each pair and can directly output labelings on each pixel. In this project, we propose a technique similar to IIC to provide both neuroanatomy segmentations and lesion segmentations on brain MR images in an unsupervised manner.

The input to our system is a slice of a brain MRI. The output to our system consists of two segmentation masks: one neuroanatomy semantic mask decomposing the brain image into its anatomical components, and another lesion binary mask indicating the presence of brain tumors.

4 Challenges

In general the task of image segmentation is very hard. Traditional image segmentation comprise of various edge-based and region-based methods [2]. However, these methods are not robust and do not generalize well across different datasets. In terms of the topics covered in class, deep learning based methods like CNNs will be useful since they have been proven in research to work well across many different domains.

During the implementation of our system, one challenge we face is dealing with the uncertainty around whether we propose will be able learn from brain MRIs. Although IIC has shown to work with image distributions occurring in nature, it's unclear how well the method will transfer to MR images.

5 Dataset

Our data will mainly come from three sources: Human connectome project MS lesion segmentation challenge 2008 data from MGH

6 Baseline & Oracle

The baseline for our system is a combination of anatomy segmentation results from FreeSurfer and the lesion segmentation results from LST. The Oracle of the system is naturally the segmentation labels provided by the radiologists. The gap between them are

Baseline Whole brain segmentation: FreeSurfer (TOO HARD???) Lesion Segmentation: <https://www.applied-statistics.de/lst.html>

Oracle: Whole brain segmentation: Radiologist??? Lesion Segmentation: Radiologist

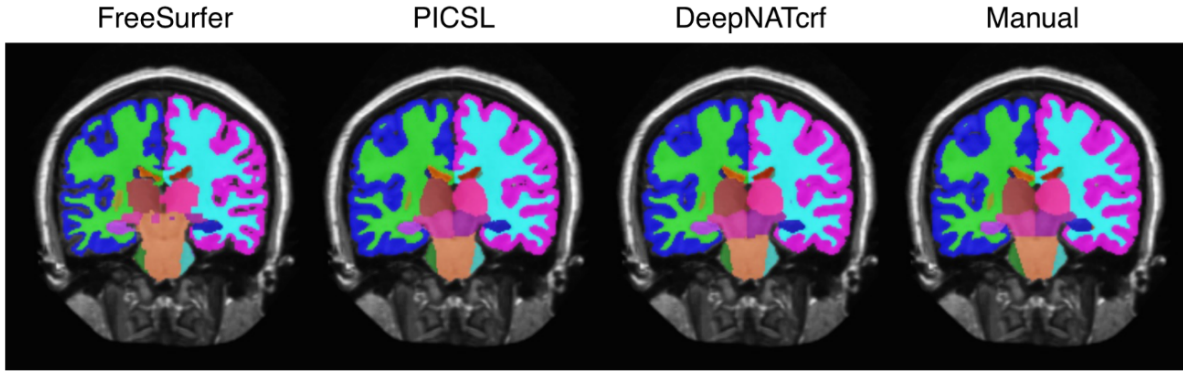


Figure 8: Example segmentations for FreeSurfer, PICSL, and DeepNATcrf together with the corresponding manual segmentation. FreeSurfer shows the largest variations with respect to the manual segmentation, particularly in cortical structures and the brainstem. The results of PICSL and DeepNATcrf are highly similar to the manual segmentation.

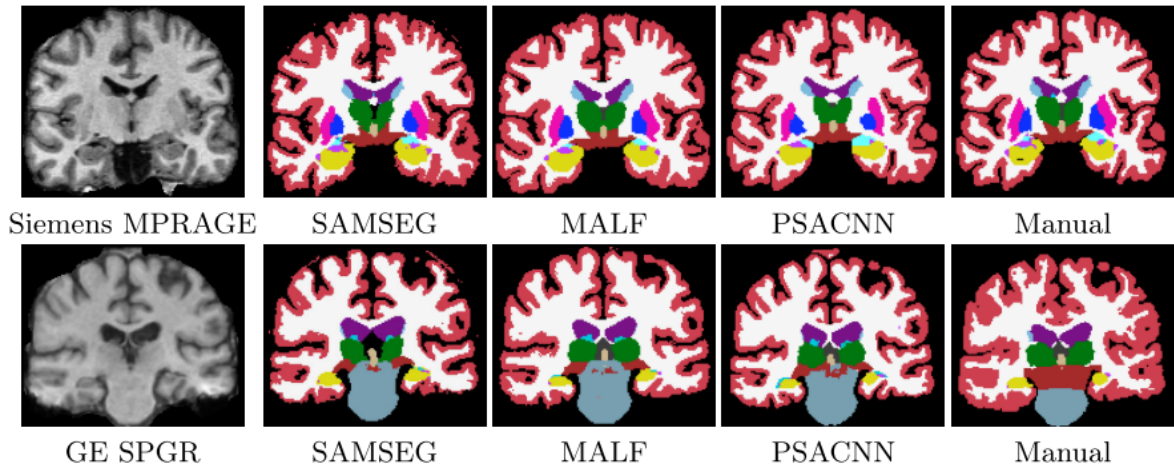


Fig. 3: Input Siemens and GE acquisitions with segmentation results from SAMSEG, MALF, and PSACNN, along with manual segmentations.

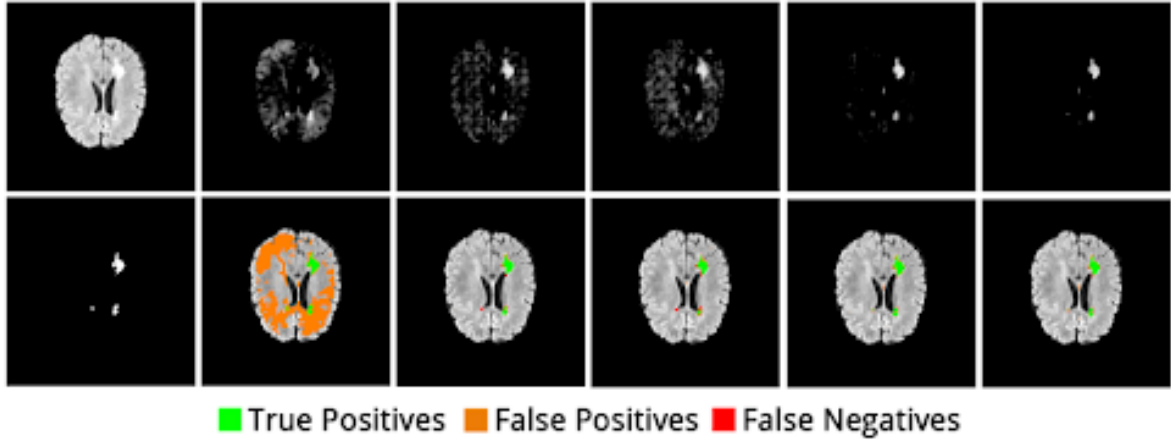


Fig. 5. 1st Column: a selected axial slice and its ground-truth segmentation; Succeeding columns show the filtered difference images (top row) and the resulting segmentation augmented to the input image (bottom row) for the following models (in order): dAE, sAE₃, sAE-GAN, sVAE and sVAE-GAN.

7 Evaluation

In order to evaluate the quality of the segmentation we can use a variety of different metrics including the Dice Coefficient, and mean IOU. For some complicated structures, we may need to have some radiologists to evaluate the results of different methods (objective scoring).

References

- [1] B. Fischl, D. Salat, E. Busa, M. Albert, M. Dieterich, C. Haselgrove, A. Kouwe, R. Kikiliani, D. Kennedy, S. Klaveness, A. Montillo, N. Makris, B. Rosen, and A. Dale, “Whole brain segmentation: Automated labeling of neuroanatomical structures in the human brain,” *Neuron*, vol. 33, pp. 341–55, 02 2002.
- [2] B. B. and R. Hegadi, “A survey on traditional and graph theoretical techniques for image segmentation,” *International Journal of Computer Applications*, pp. 38–46, 02 2014.