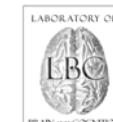


# Multi-echo EPI for resting state and activation-based fMRI

Javier González-Castillo

Section on Functional Imaging Methods, NIMH, NIH

March 24<sup>th</sup>, 2016. Texas Tech Neuroimaging Institute, Lubbock, TX.



- *Noise sources in fMRI*
- *Multi-echo fMRI as a Denoising Technique*
- *ME-ICA Denoising*
- *ME-ICA Denoising Applications*
- *Conclusions*

# Introduction to fMRI: Noise Sources

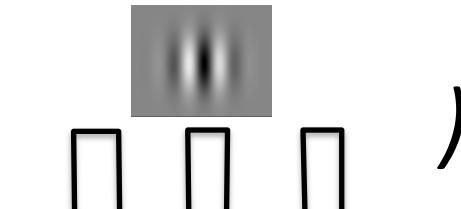
$fMRI = f($



,



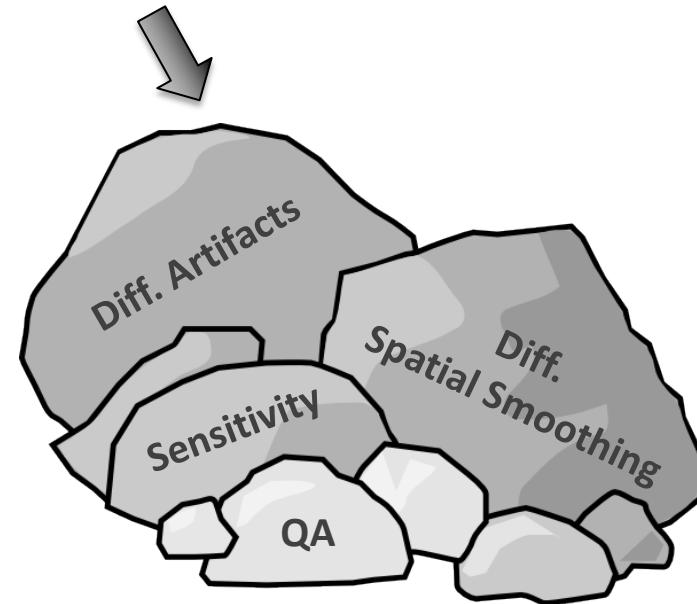
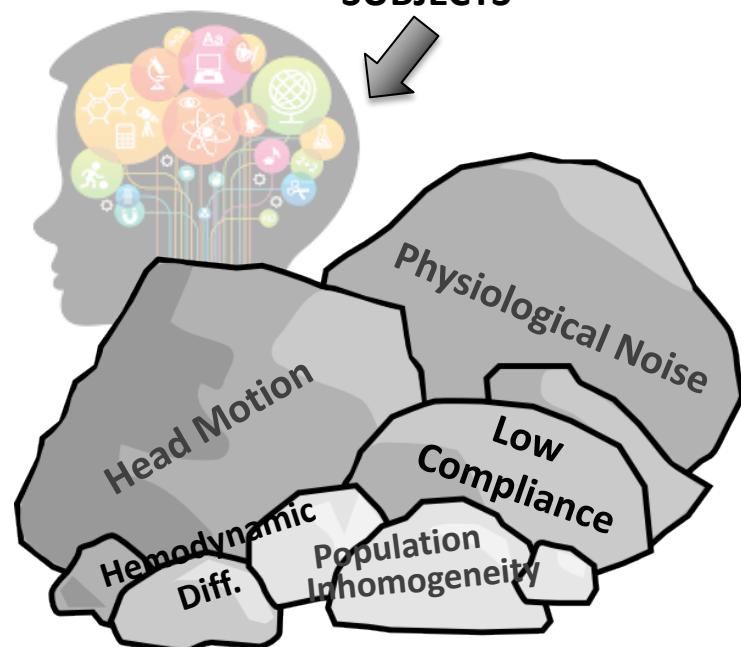
,



EXPERIMENTAL  
PARADIGM

SUBJECTS

HW  
(SCANNER)

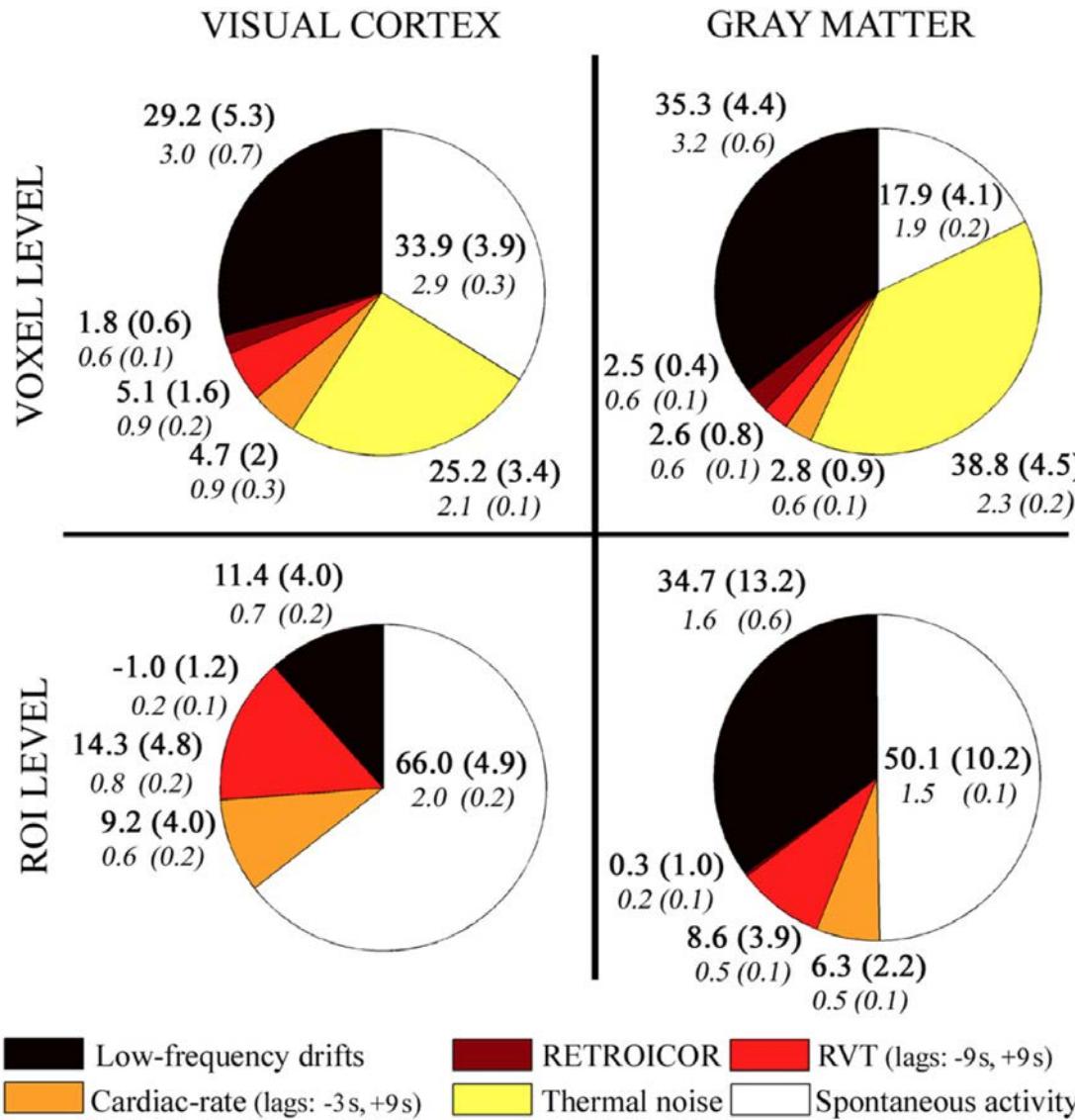


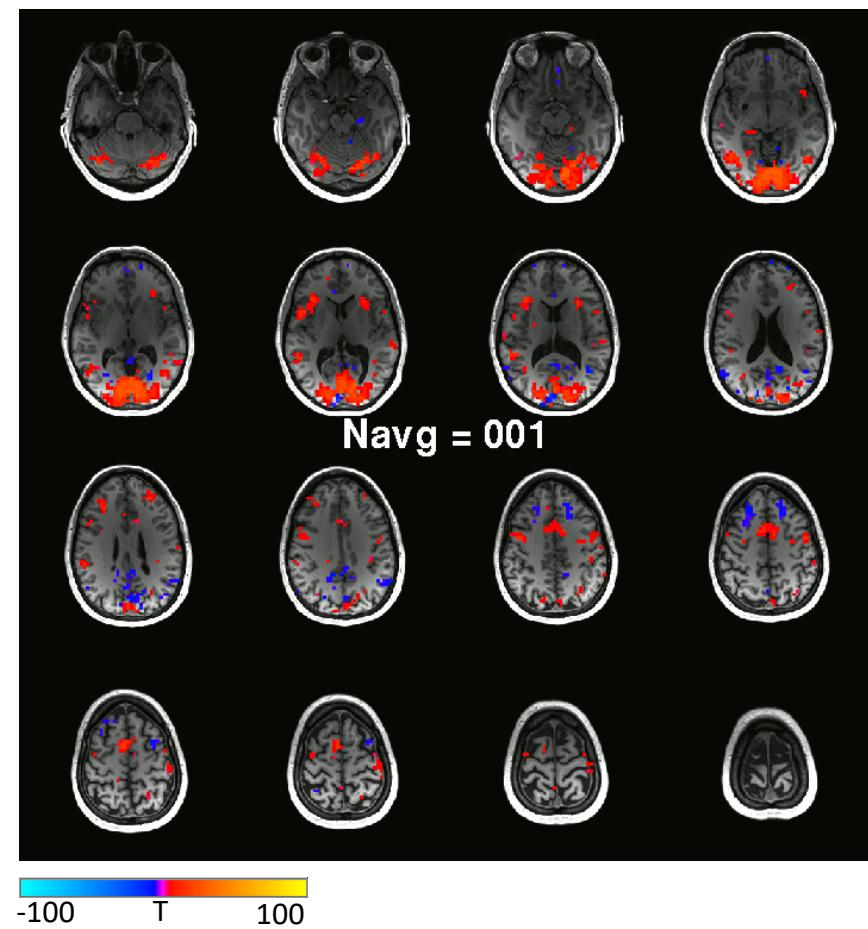
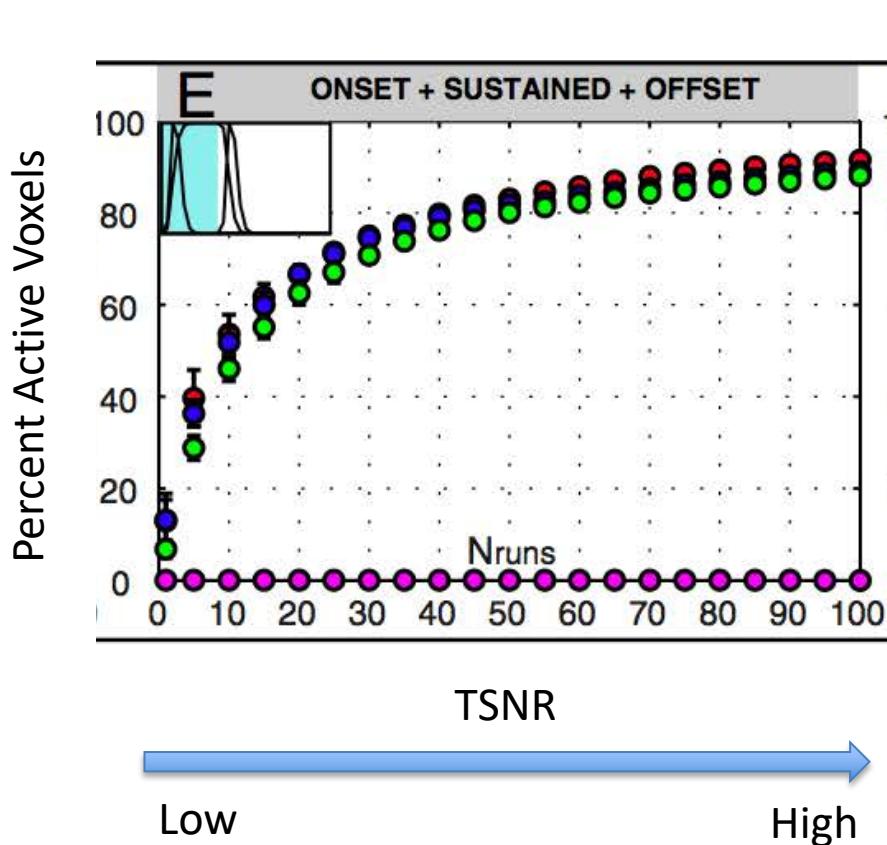
**ONLY A SUBSET OF THE SIGNAL WE MEASURE CONTAIN INFORMATION ABOUT  
NEURONAL PROCESSES**

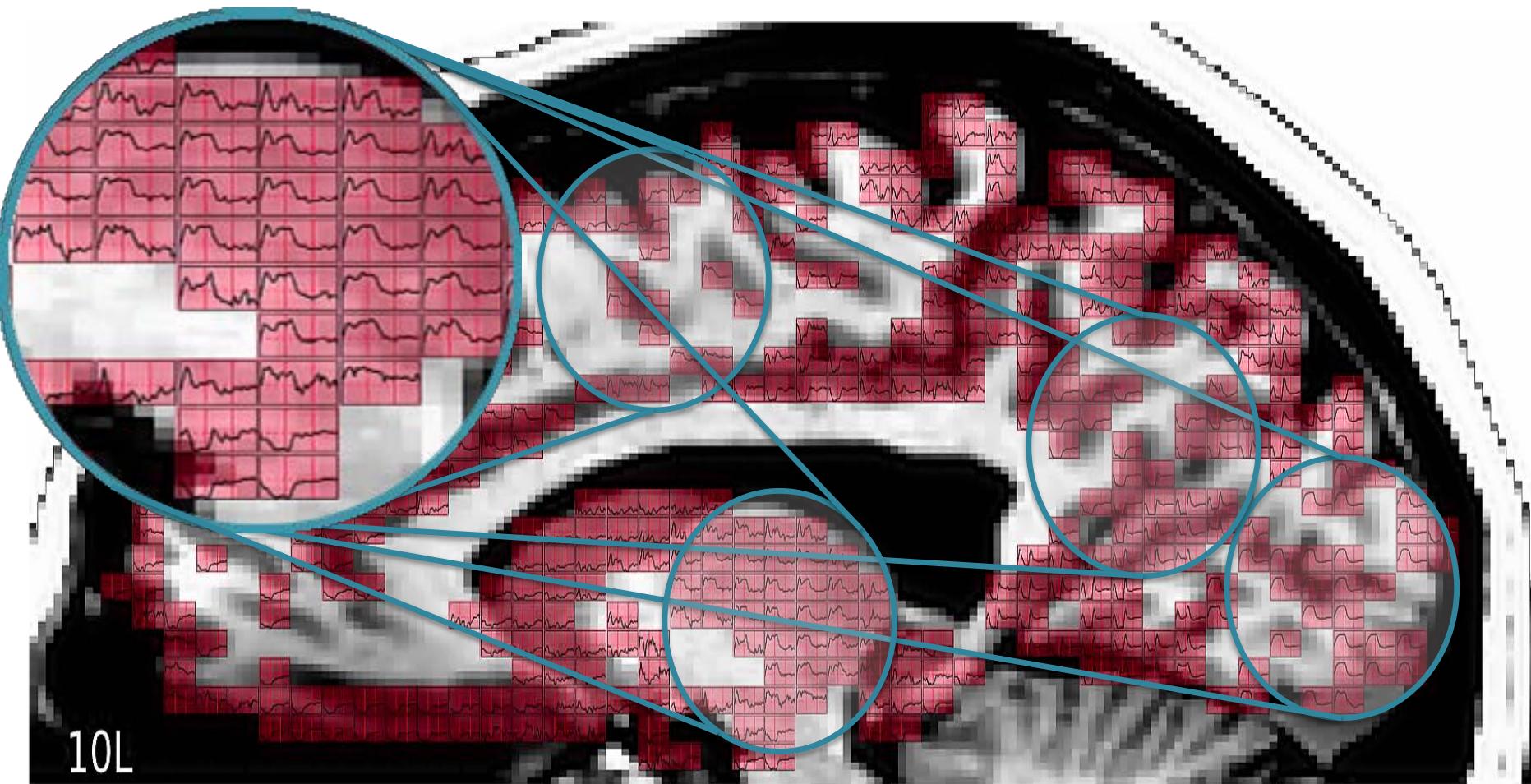
*How to best isolate and interpret this extremely valuable component of the fMRI signal?*

# fMRI Datasets have inherently low TSNR

**fMRI Time series = Signal of Interest (NEURONAL ORIGIN) + Other Fluctuations**







# fMRI Data Pre-processing

## NOISE SOURCE



Slow Signal Drifts



Head Motion



Physiological Noise

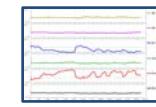


Localized HW Instabilities

## MODEL REGRESSOR



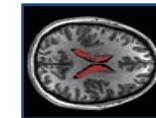
Legendre Polynomials



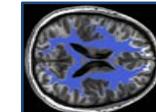
Head Motion Estimates



RETROICOR + RVT



Lateral Ventricle Regressors



Local WM Regressor



# Multi-Echo fMRI & ME-ICA Denoising

MEICA is not only a pre-processing technique, it also requires data to be acquired differently.

1

MULTI-ECHO DATA  
ACQUISITION

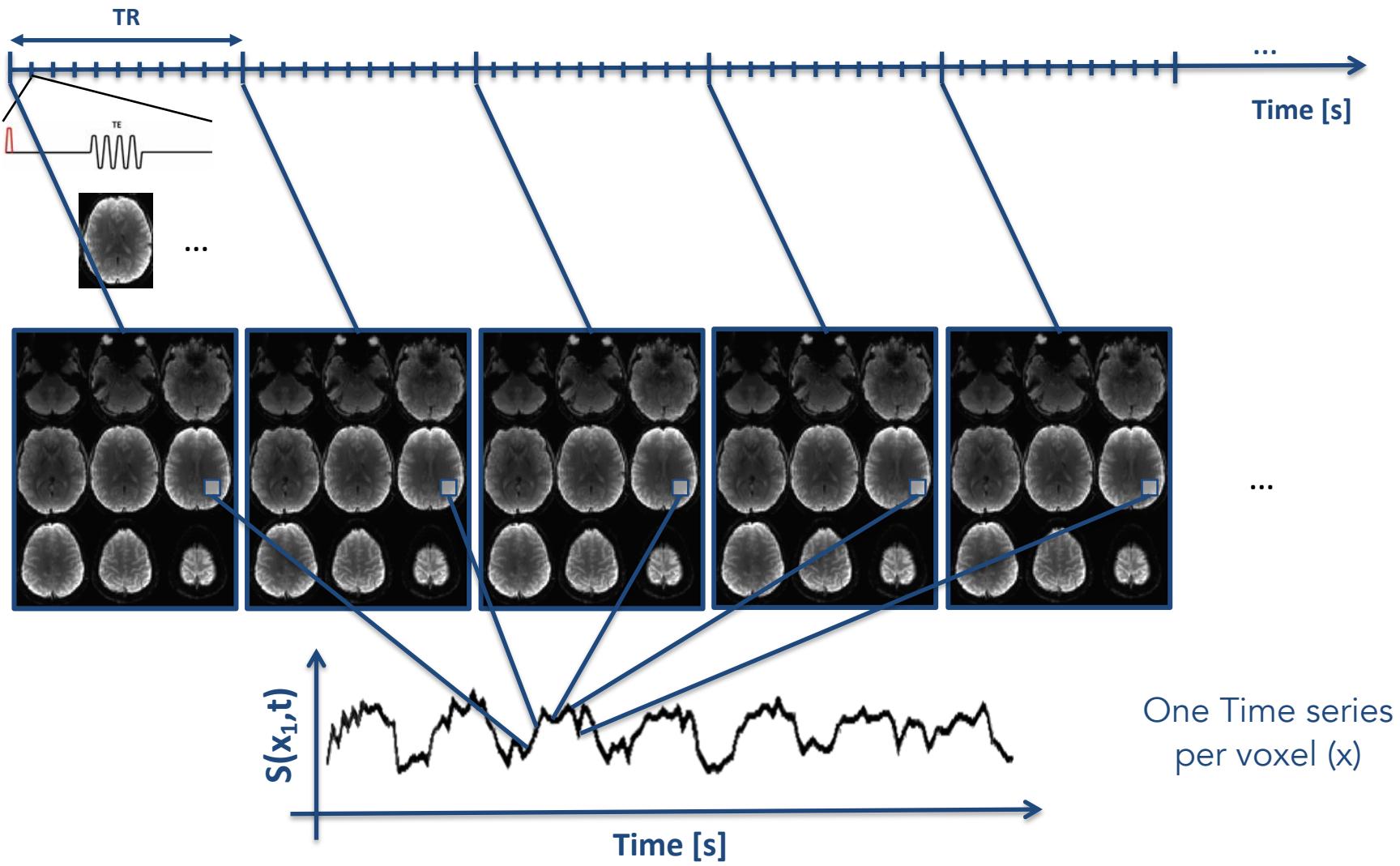
2

ICA DECOMPOSITION TO OBTAIN  
SPATIALLY INDEPENDENT SOURCES  
OF FLUCTUATION IN THE DATA

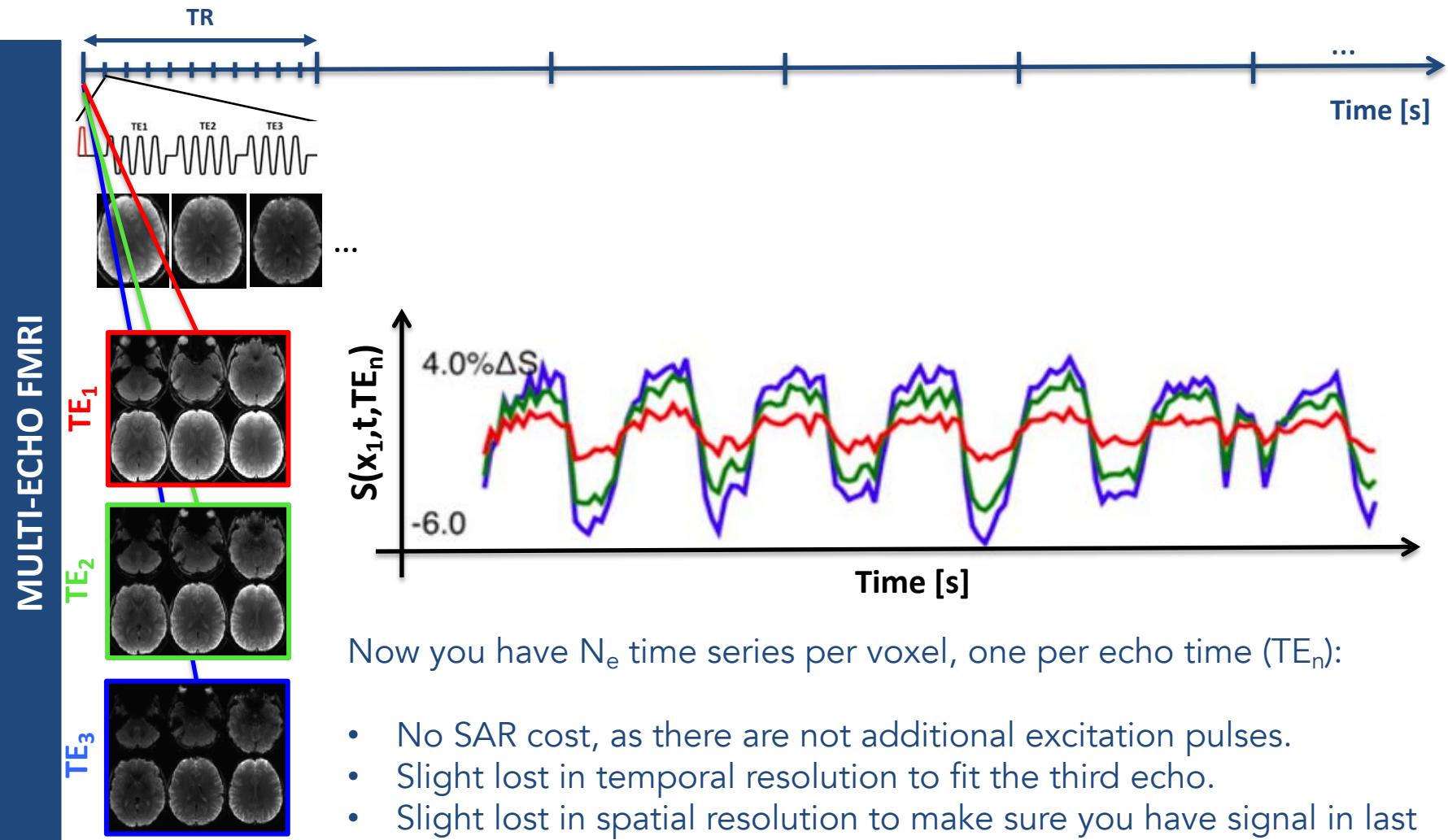
3

AUTOMATIC CLASSIFICATION OF ICA  
COMPONENTS INTO "GOOD OR BAD"  
BASED ON A PHYSICALLY INFORMED ECHO-  
DEPENDENCE MODEL OF THE SIGNALS

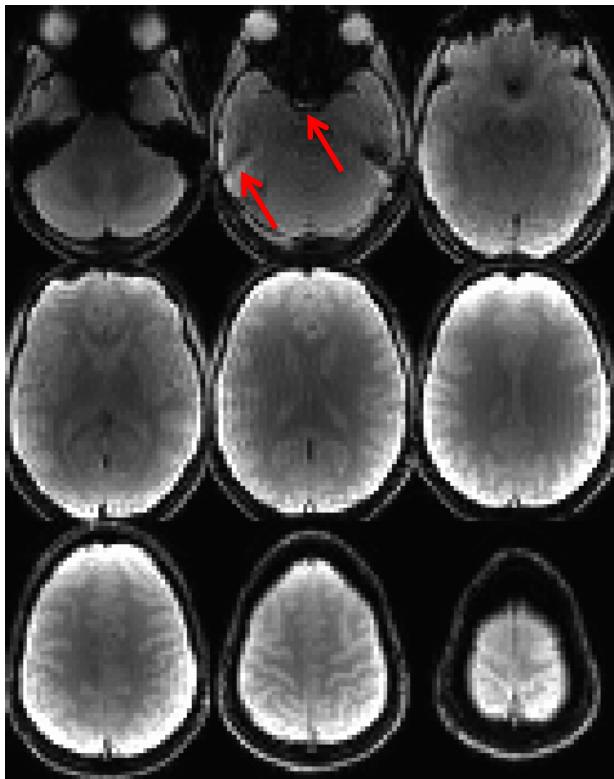
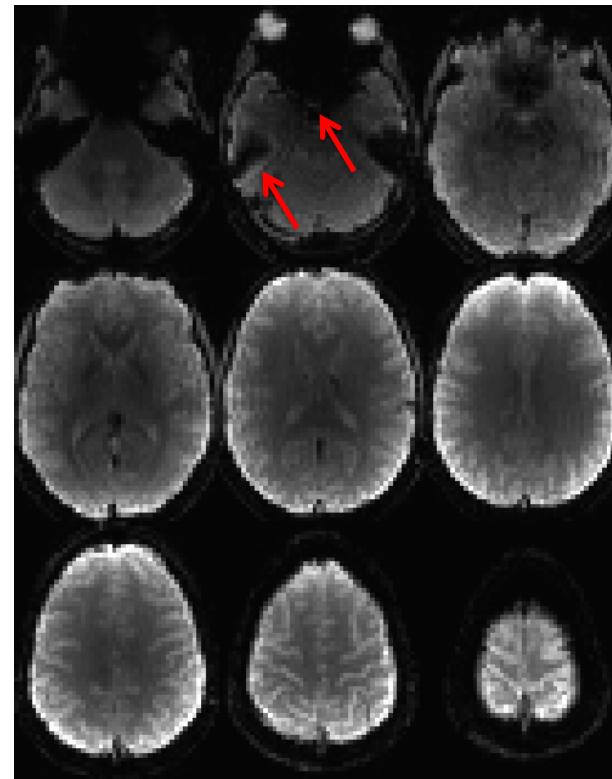
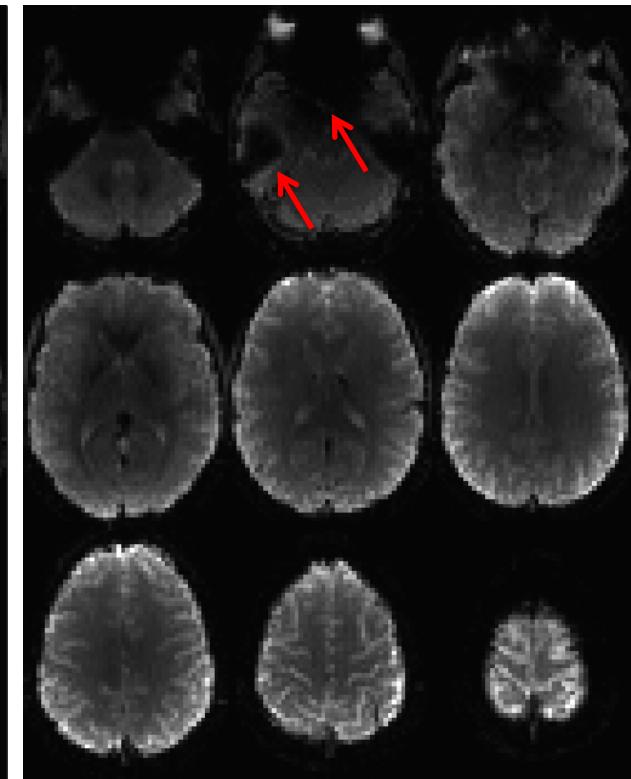
# Single-Echo Data Acquisition



# Multi-Echo Data Acquisition



## Multi-Echo Data

 $TE_1$  $TE_2$  $TE_3$ 

We have  $N_e$  pseudo-concurrent measurements → why not simply combine them to reduce uncorrelated white noise present in each individual measurement?

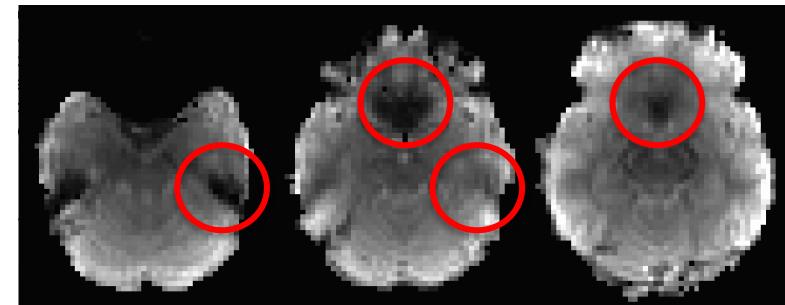
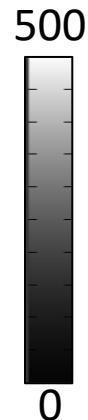
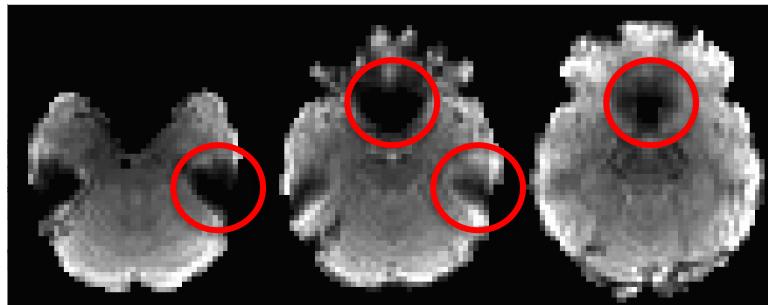
### Weighted Summation

$$\hat{S}(x, t) = \sum_{n=1}^N S(x, t, TE_n) \cdot w_v(TE_n)$$

$$w_v(TE_n) = \frac{TE_n e^{-TE_n/T_{2,v}^*}}{\sum_n TE_n \cdot e^{-TE_n/T_{2,v}^*}}$$

- Helps to spatially maximize CNR and also to recover some signal level in regions affected by drop-out.

Posse et al., MRM 1999



OPTIMALLY COMBINED

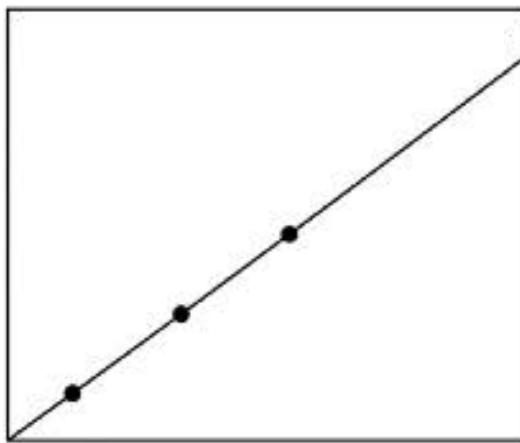
# ME-ICA: Echo-Dependence Model

fMRI Data = BOLD-Like Components + Non-BOLD-Like Components

(Neuronal Origin)

(Nuisance/Artifacts)

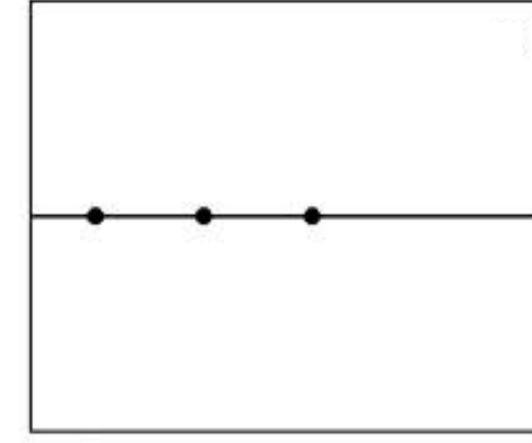
$$\Delta S(x, TE) / S(x, t, TE)$$



Echo Time

BOLD-Like Components have a linear dependence with echo time, in terms of signal percent change.

$$\Delta S(x, TE) / S(x, t, TE)$$

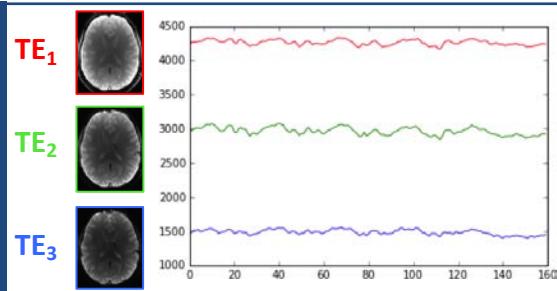


Echo Time

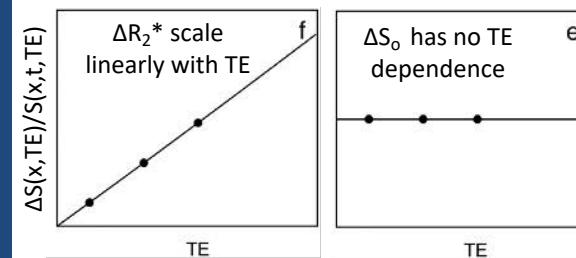
Non-BOLD-Like Components are independent of echo time, in terms of signal percent change

# Echo Time (TE) Dependence Analysis

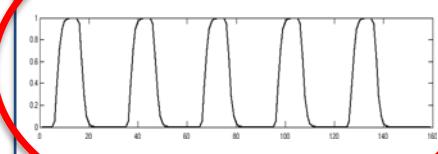
## MULTI-ECHO DATASET



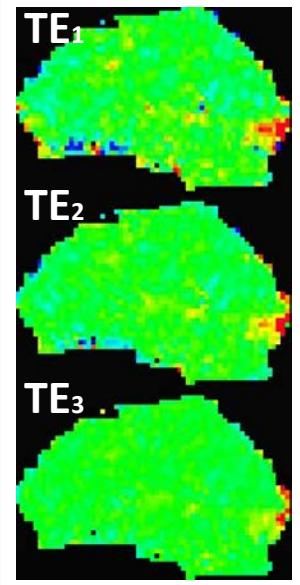
## TE-DEPENDENCE MODEL



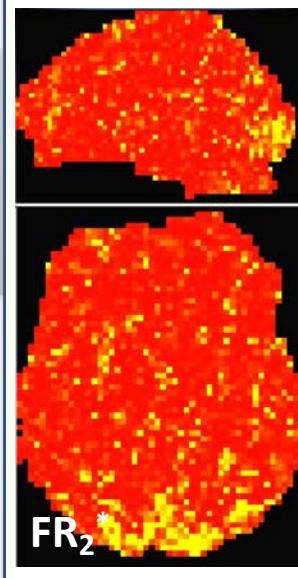
## TIMESERIES OF INTEREST



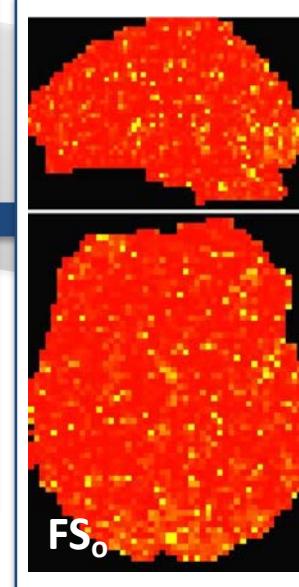
### [1] Voxel-wise Fit against all TEs



### [2] Voxel-wise Goodness of Fit to R₂\* Model



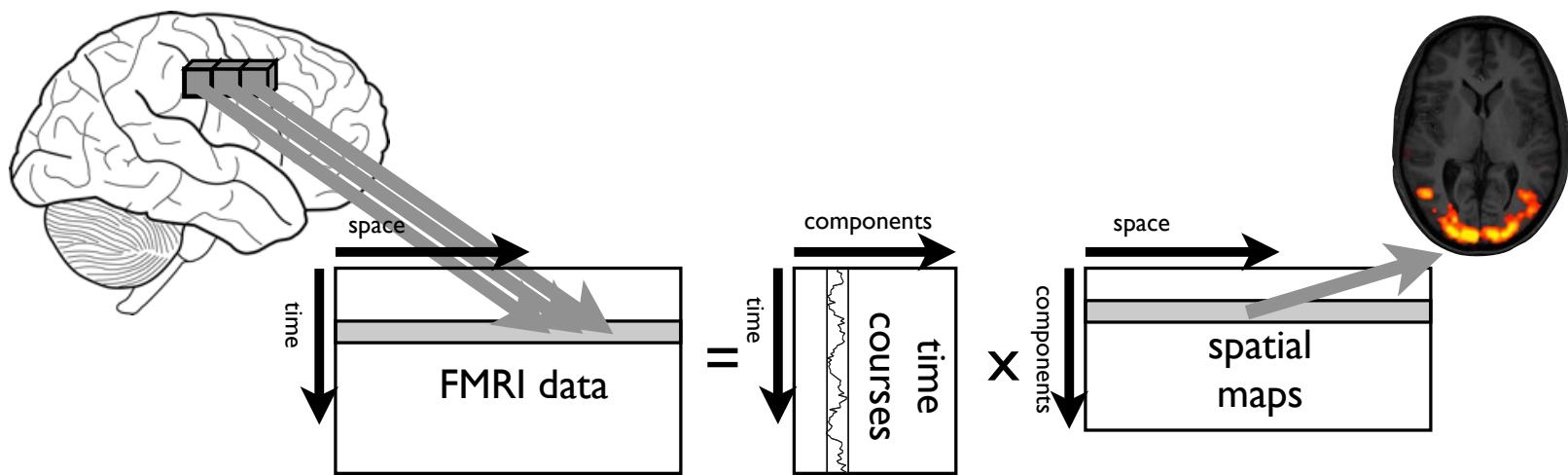
### [3] Voxel-wise Goodness of Fit to S₀ Model



### [4] Compute Avg. Metric for each model

$$\kappa = \frac{\sum_{AllVoxels} z_v^2 F_{v,R_2^*}}{\sum_{AllVoxels} z_v^2} = 98.41$$

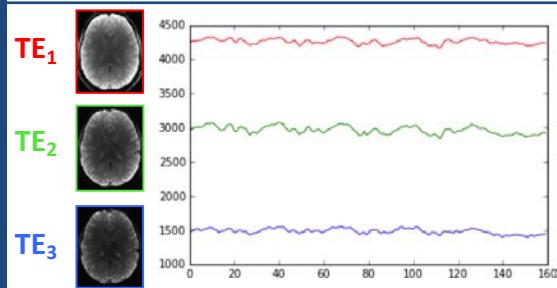
$$\rho = \frac{\sum_{AllVoxels} z_v^2 F_{v,S_0}}{\sum_{AllVoxels} z_v^2} = 26.02$$



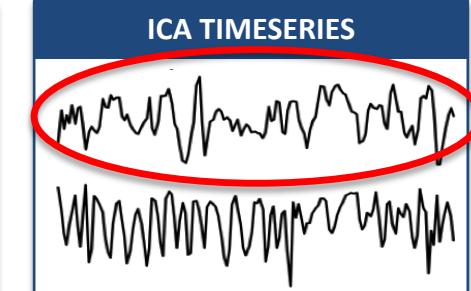
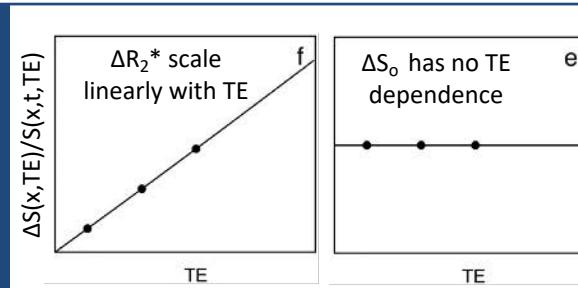
Data is represented as a 2D matrix and decomposed into factor matrices (or modes)

# ME-ICA: How it works

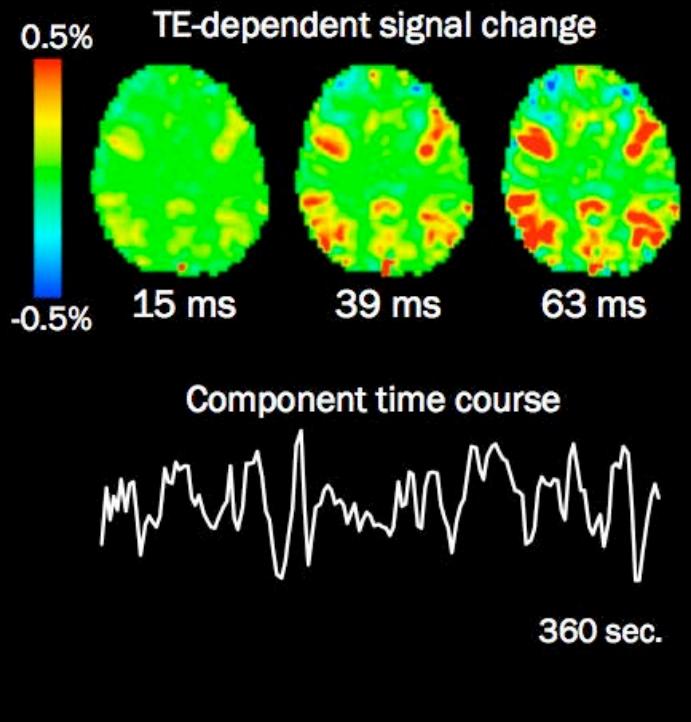
MULTI-ECHO  
DATASET



TE-DEPENDENCE  
MODEL



(a) Functional Network Component

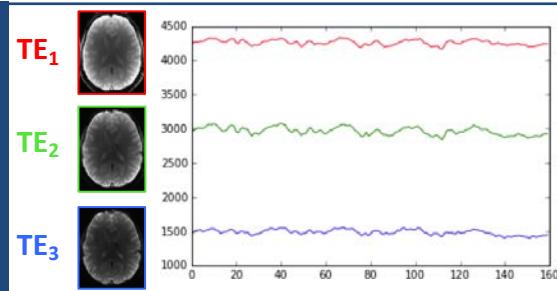


Kappa ( $\kappa$ ) = 210

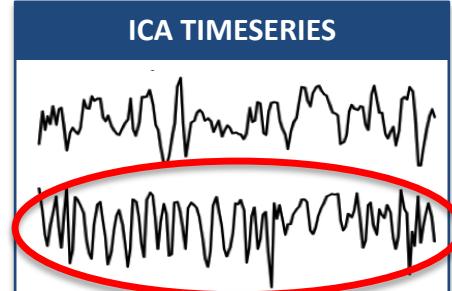
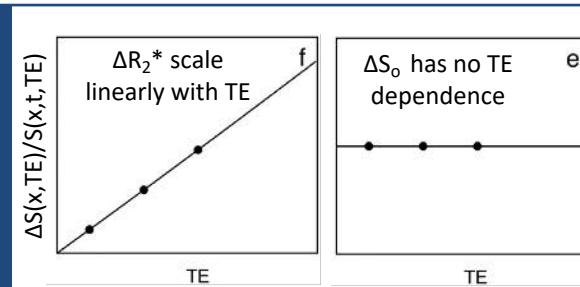
Rho ( $\rho$ ) = 10

# ME-ICA: How it works (2)

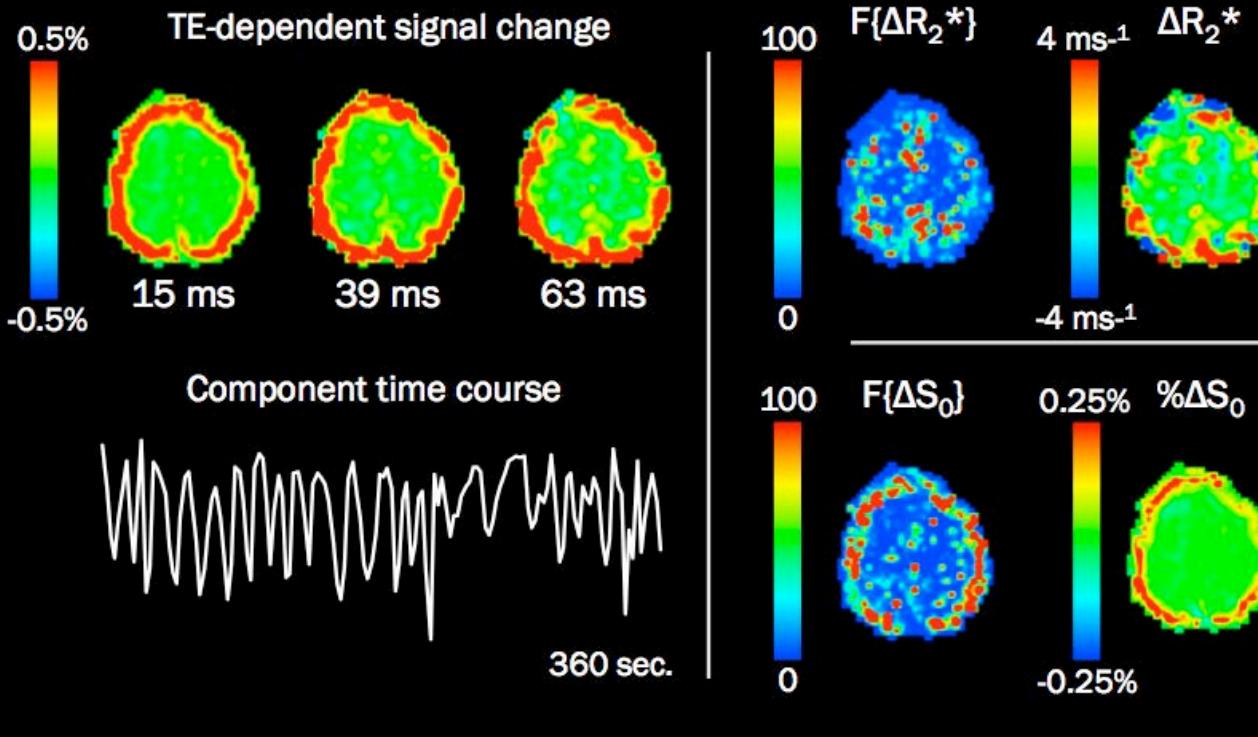
## MULTI-ECHO DATASET



## TE-DEPENDENCE MODEL

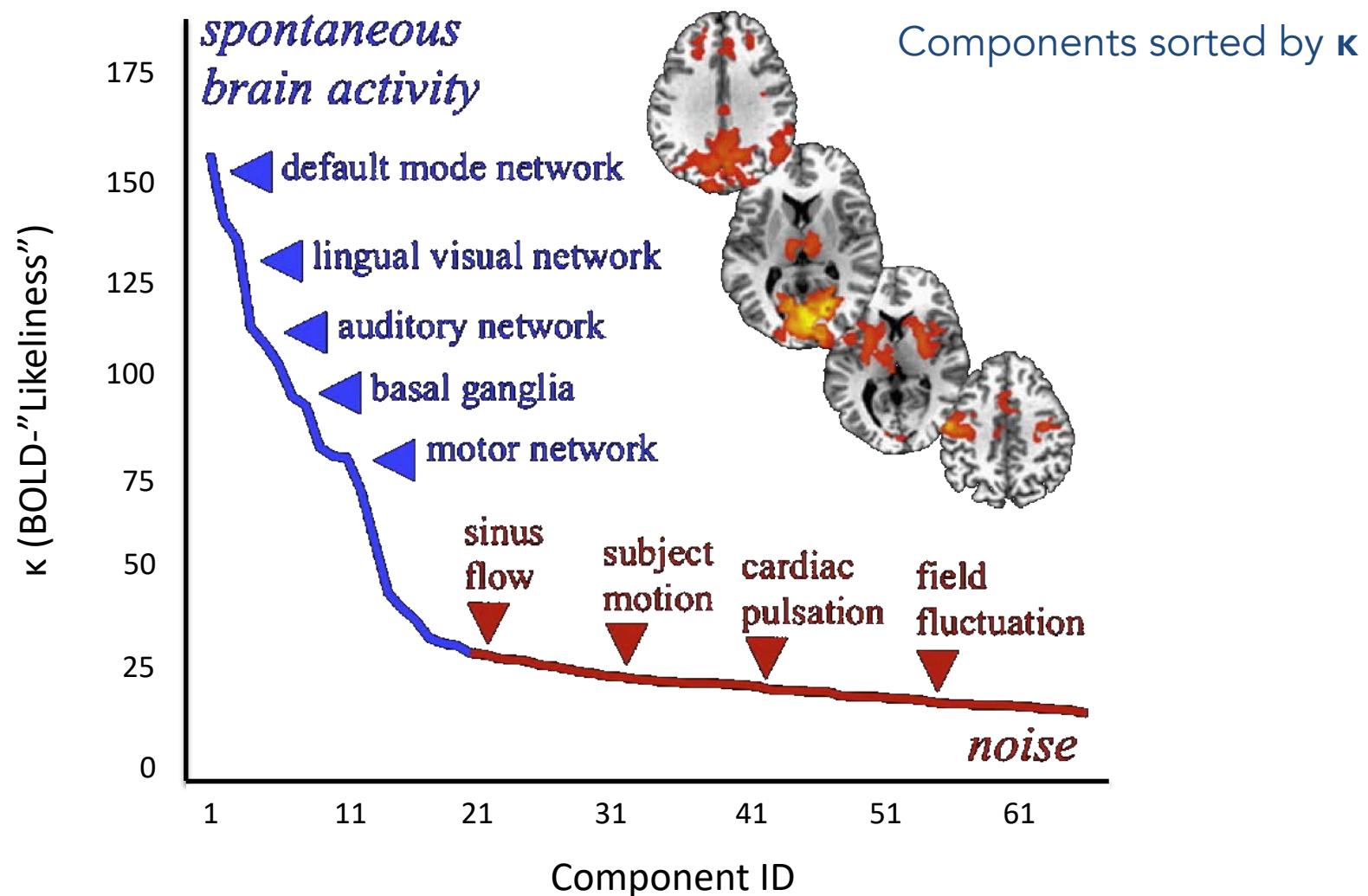


### (b) Artifact Component

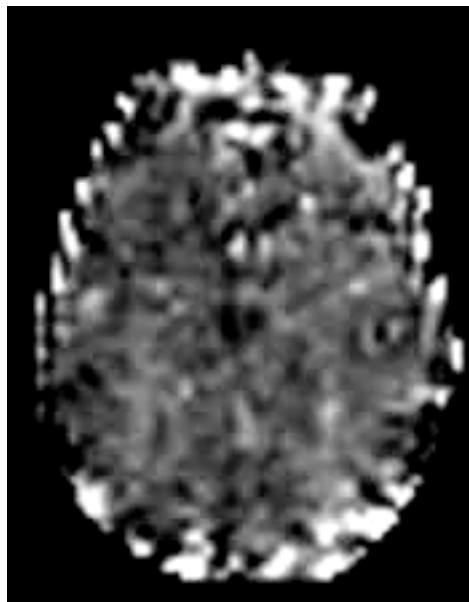


Kappa ( $\kappa$ ) = 32

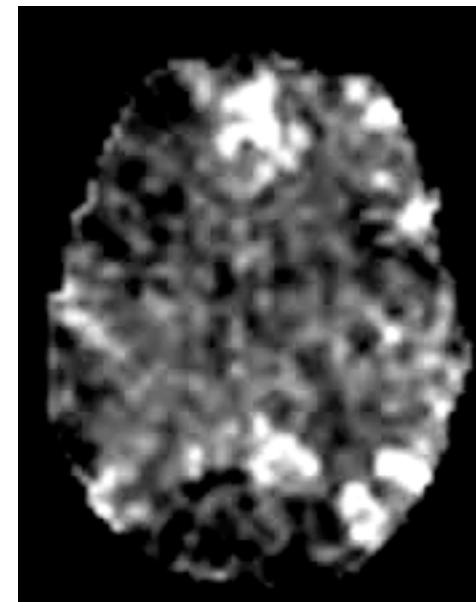
Rho ( $\rho$ ) = 81



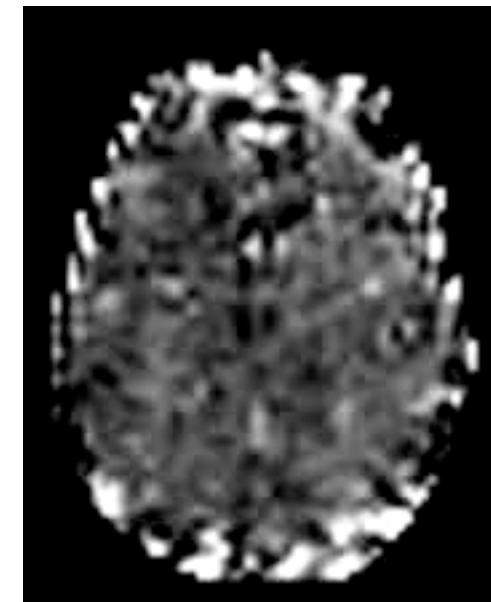
# ME-ICA: Outcome



=



+



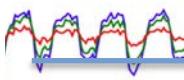
fMRI Timeseries

=

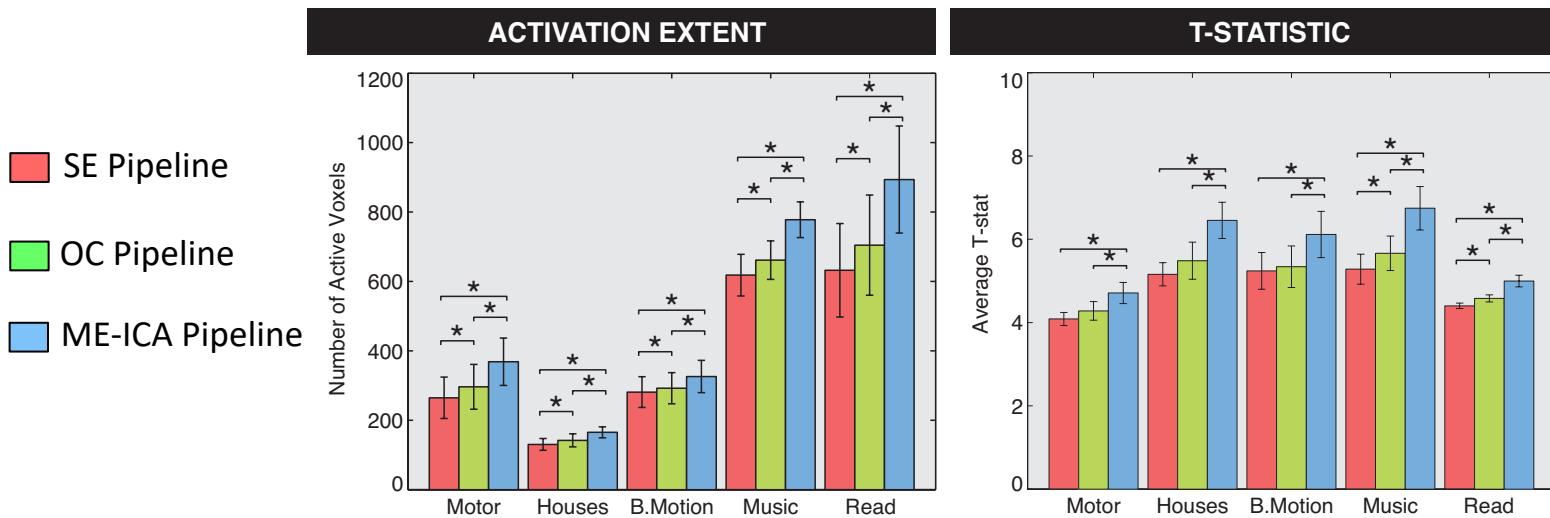
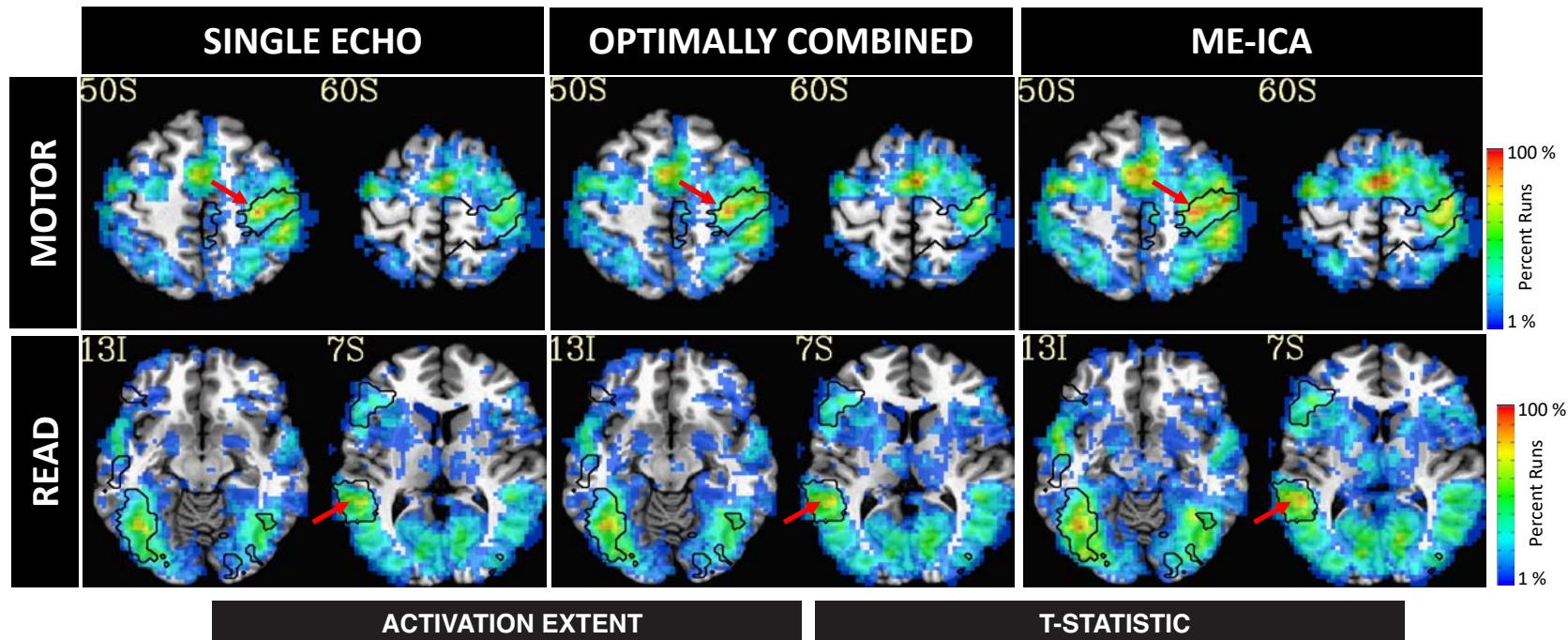
BOLD

+

NON BOLD



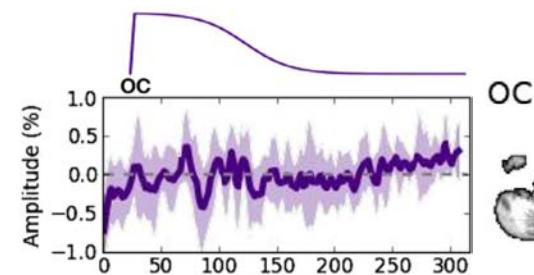
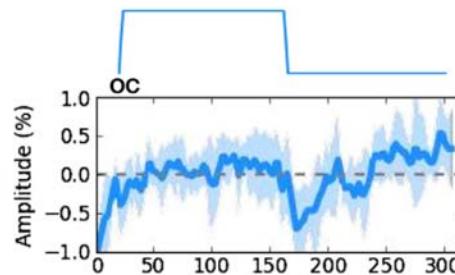
# Multi-Echo fMRI – Improvements for task-based data



# ME-ICA & Ultra-slow Experimental Designs

Detection of activity in very slow paradigms (2 min long blocks)

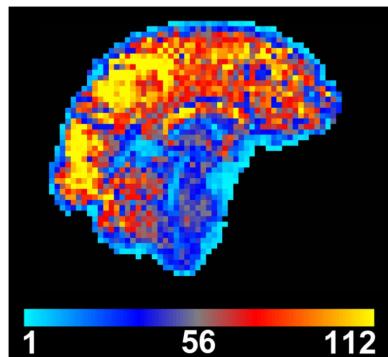
OC



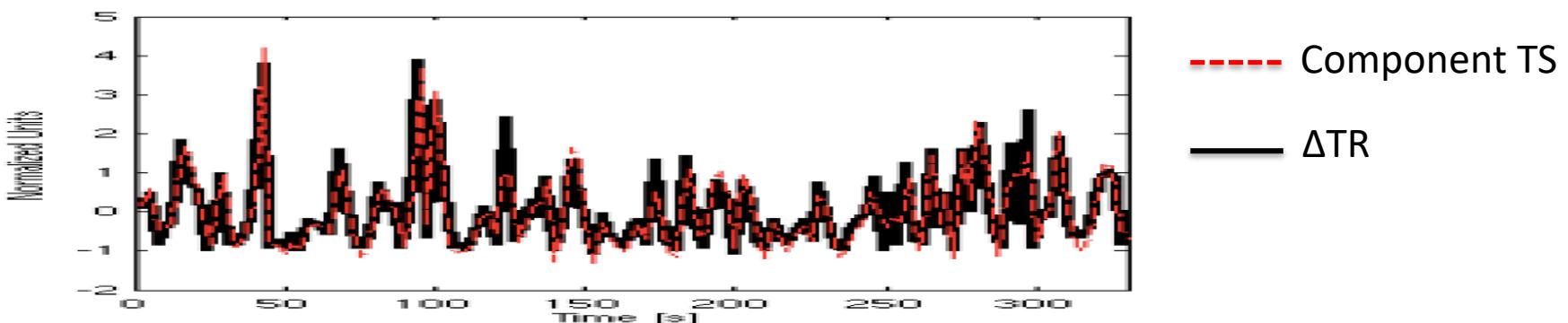
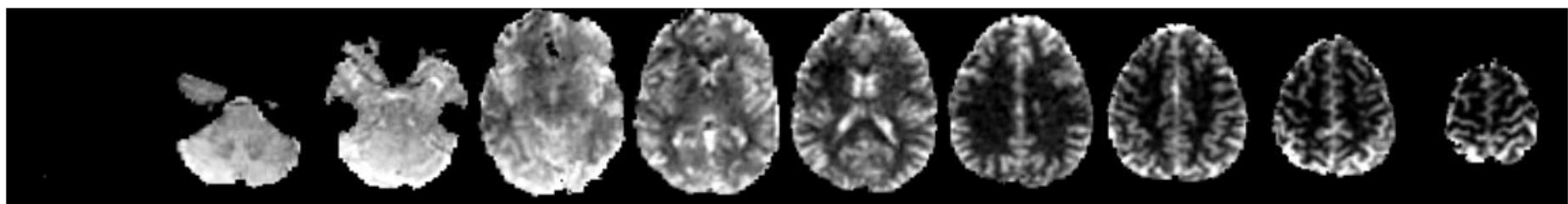
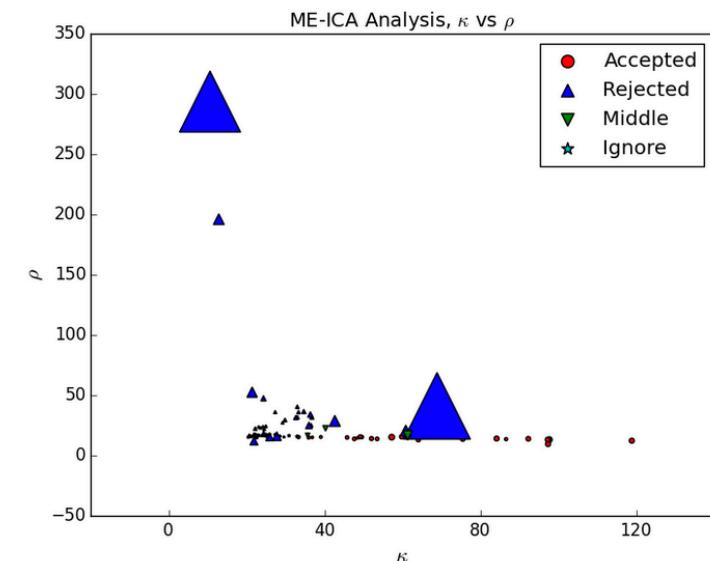
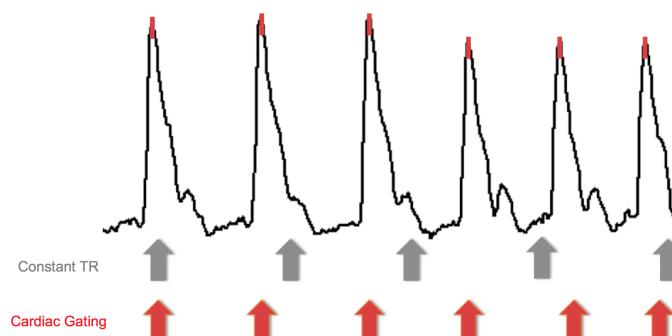
OC

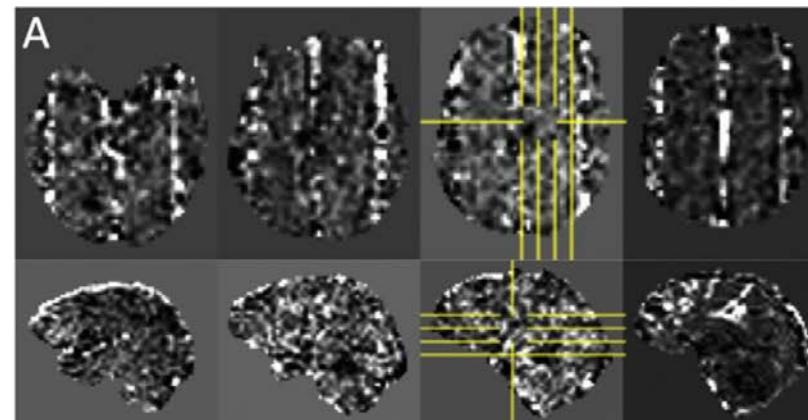


## ME-ICA &amp; Cardiac Gated fMRI

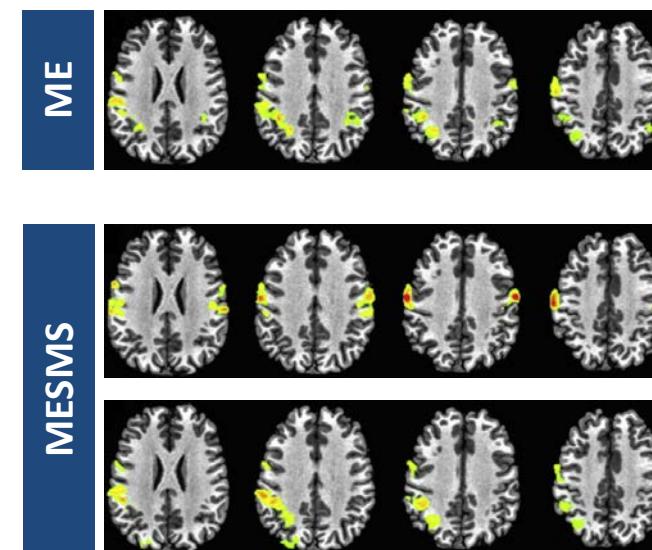
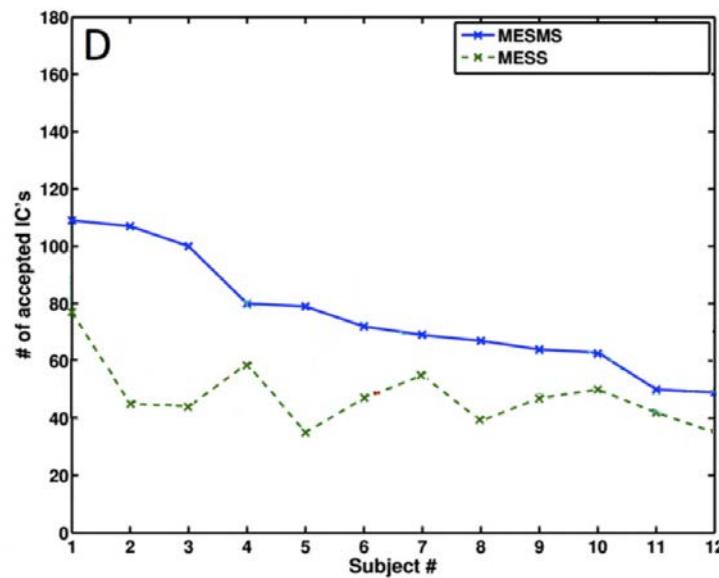


Brooks et al. 2014





Non-BOLD Component: MSS Artifact



Number of BOLD-like components significantly larger for MESMS

- Multi-echo fMRI allows to capture additional information with minimal costs in terms of temporal and spatial resolution.
- Such additional information can be used to:
  - Increase CNR in drop-out regions (e.g., Optimal Combination of Echoes).
  - Automatically separate BOLD-like from Non-BOLD-like components (ME-ICA).
- ME-ICA is a promising denoising methodology that combines ICA with TE-Dependence Analysis:
  - Can substantially improve the SNR of the data → Quality of the results.
  - Still under development.

# Acknowledgements

## Section on Functional Imaging Methods

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Daniel Glen  
Richard Reynolds  
Gang Chen



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Catie Chang

