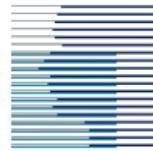


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Cardiac Electrophysiology
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Learning to Predict Global Atrial Fibrillation Dynamics from Sparse Measurements

Temporal Graph Reading Group

Alexander Jenkins
27/03/2025

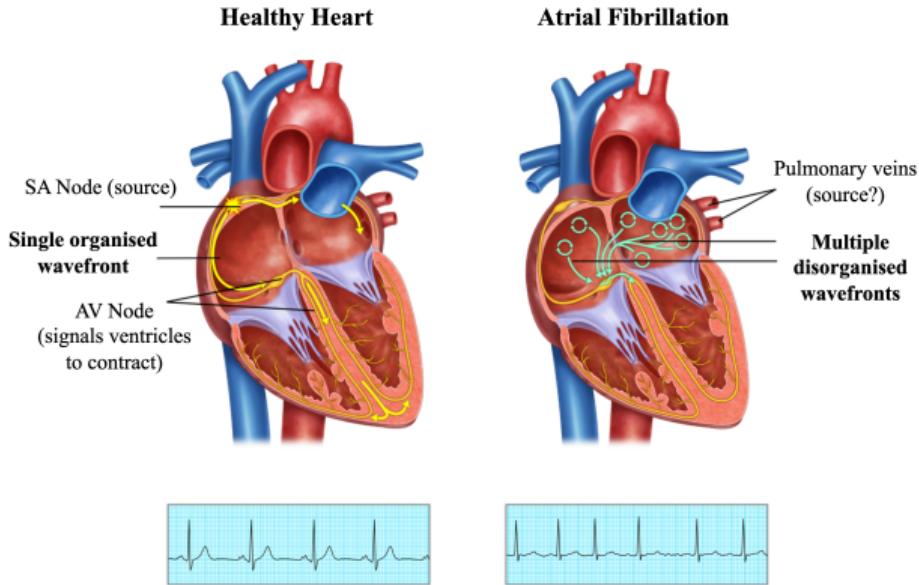
Atrial Fibrillation (AF)

Prevalence

- Most common cardiac arrhythmia with lifetime risk of 1 in 3.
- Affects 37.5 million people worldwide (0.5% of global population).
- Projected 60% rise by 2050.

Burden

- Major cause of stroke, heart failure, and death.
- Major cost to global healthcare (2.4% of annual UK healthcare budget).



Propagation Dynamics in AF

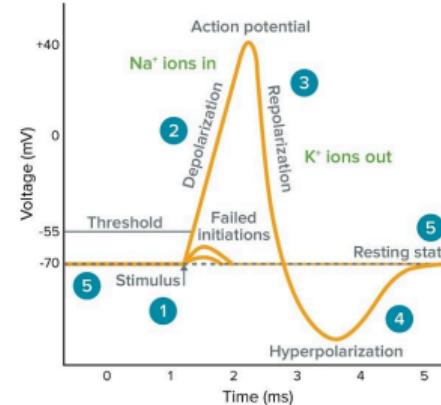
The Local Level

The Cable Equation:

$$\frac{\partial V}{\partial t} = \nabla \cdot (D \nabla V) - \frac{I_{ion}(V; y)}{C_m}$$

$$\frac{\partial y}{\partial t} = g(V; y)$$

- $V(x, y, z, t)$: Membrane potential
- $\nabla \cdot (D \nabla V)$: Diffusion/coupling term
- I_{ion} : Total ionic current across membrane
- C_m : Membrane capacitance
- y : Vector of various ionic channel currents
- $g(V; y)$: Functions governing channel dynamics



Properties:

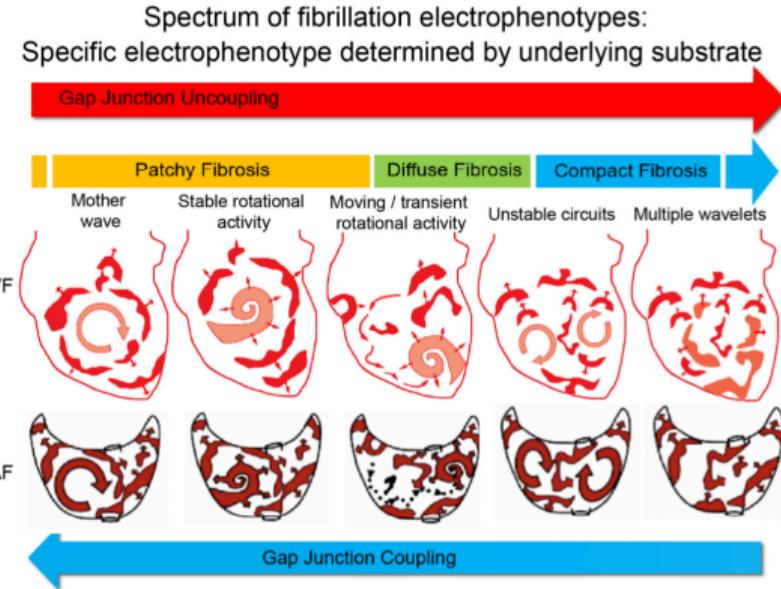
- Neighbouring spatial regions are electrically coupled.
- Anisotropic diffusion through the $\nabla \cdot (D \nabla V)$ term.
- Local D and $\frac{I_{ion}}{C_m}$ affect global wave patterns.
- Threshold-dependent activation and recovery dynamics.

Propagation Dynamics in AF

The Global Level

The Mechanisms Sustaining AF

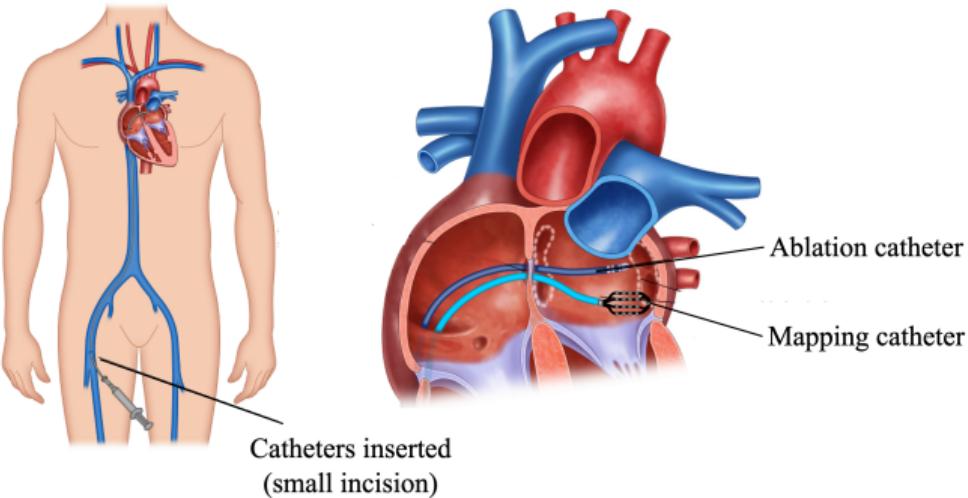
- Heterogeneous disorder with diverse electrophenotypes.
- Spatio-temporal dynamics vary in a spectrum from organised to disorganized chaos.
- Triggers that sustain the AF dynamics may originate from the pulmonary veins.



AF Ablation & The Need for Accurate Mapping

The Challenge of AF Ablation

- Electrical isolation of the pulmonary veins from the left atria has success rates at best 50% at 5 years for persistent AF (Scherr et al. 2015).
- One-size-fits-all approach for a heterogeneous disease.
- Personalised treatment requires accurate identification of the fibrillation mechanism.

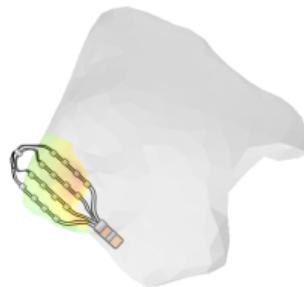


Mapping Limitations

- Current technologies face a trade-off in achieving global coverage and high resolution mapping.

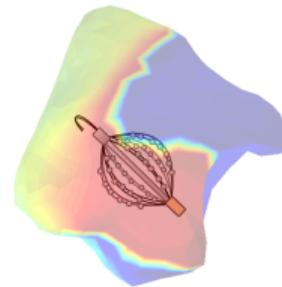
The Trade-off in AF Mapping

Contact vs. Non-Contact Mapping



Contact Mapping

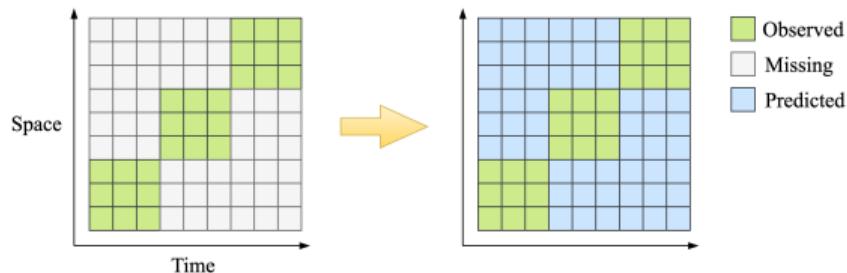
- ✓ Precise measurements at contact locations.
- ✓ Standard clinical approach.
- ✗ Limited coverage (10% of atrium).
- ✗ Sequential collection process.
- ✗ Recordings cannot be sensibly stitched in AF.



Non-Contact Mapping

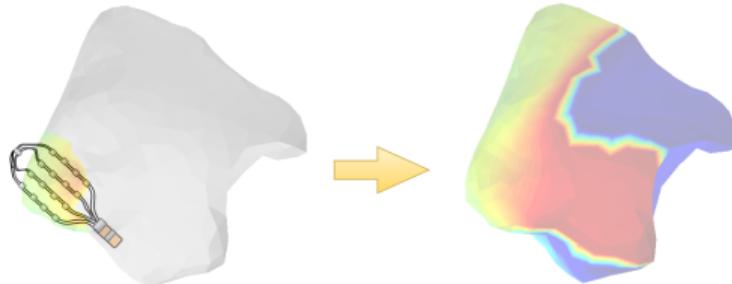
- ✓ Global coverage of atrial surface.
- ✓ Simultaneous whole-chamber recording.
- ✗ Low spatial resolution.
- ✗ Not routinely used clinically.
- ✗ Increased procedural risk and cost.

Introducing Imputation Mapping



Spatio-Temporal Imputation Framework

- Contact mapping provides sparse observations (10% of atrium).
- Formulate imputation mapping as a matrix completion problem (space vs. time).
- Learn spatio-temporal patterns from observed values to reconstruct missing regions.
- Leverage atrial surface geometry as an inductive bias in the processing.

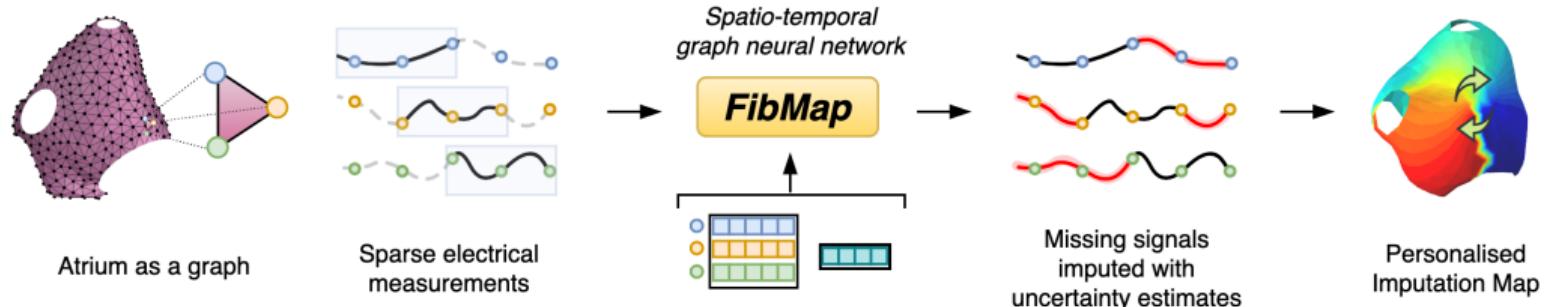


Key Challenges for AF Imputation

- Propagating information across highly sparse observations.
- Managing unknown parameters affecting AF dynamics.
- Balancing personalisation vs. generalisation.
- Efficiently training and adapting to new patients.
- Quantifying uncertainty in reconstructions.

Imputation Mapping via FibMap

A Graph Recurrent Neural Network for AF Mapping



1) Personalise

Patient-specific parameters capture unique AF dynamics.

2) Encode

Signal values, mask, and patient-specific parameters transformed to a hidden representation.

3) Process

Bidirectional graph-RNN propagates information across space and time from observed regions.

4) Decode

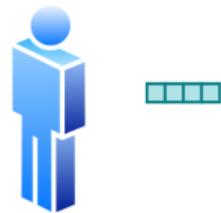
Spatio-temporal representations from both directions combined to reconstruct missing signals.

Imputation Mapping via FibMap

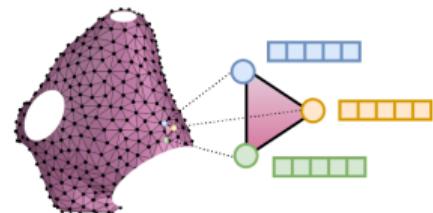
Personalise

Balancing Globality and Locality in GRNNs

- GRNNs are inherently global models.
- Global models may struggle to capture node (and patient)-specific dynamics.
- Node embeddings allow for a hybrid global-local approach (Cini et al. 2023).



Patient embeddings
Capture properties of the patient
(e.g. blood pressure, ...)



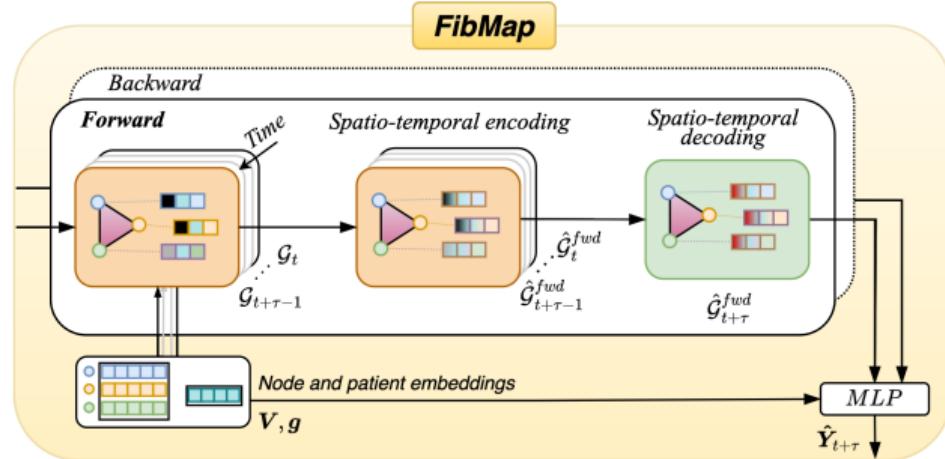
Node embeddings
Capture properties of the tissue
(e.g. conductivity, ...)

Personalising FibMap

- Node embeddings $V^{(p)} \in \mathbb{R}^{N \times q}$ capture latent spatial tissue properties.
- Patient embeddings $g^{(p)} \in \mathbb{R}^r$ capture global dynamics specific to each patient.
- May provide interpretable insights for electrophenotyping.

Imputation Mapping via FibMap

Encode, Process, Decode



Encode: Transform inputs into initial hidden representation

$$\mathbf{H}_t^0 = \text{MLP}_{\text{enc}}([\mathbf{X}_t^{(p)} \odot \mathbf{M}_t^{(p)} \| \mathbf{M}_t^{(p)} \| \mathbf{g}^{(p)} \| \mathbf{V}^{(p)}]) \quad (1)$$

$\mathbf{X}_t^{(p)}$: observations, $\mathbf{M}_t^{(p)}$: masks,
 $\mathbf{g}^{(p)}$: patient embeddings, $\mathbf{V}^{(p)}$: node embeddings.

Process: K gated-graph RNN layers

$$\begin{aligned}\mathbf{Z}_t^k &= \mathbf{H}_{t-1}^k, \\ \mathbf{R}_t^k &= \sigma(\text{MP}_r^k([\mathbf{Z}_t^k \| \mathbf{H}_{t-1}^k], \mathcal{E})), \\ \mathbf{U}_t^k &= \sigma(\text{MP}_u^k([\mathbf{Z}_t^k \| \mathbf{H}_{t-1}^k], \mathcal{E})), \\ \mathbf{C}_t^k &= \tanh(\text{MP}_c^k([\mathbf{Z}_t^k \| \mathbf{R}_t^k \odot \mathbf{H}_{t-1}^k], \mathcal{E})), \\ \mathbf{H}_t^k &= \mathbf{U}_t^k \odot \mathbf{H}_{t-1}^k + (1 - \mathbf{U}_t^k) \odot \mathbf{C}_t^k\end{aligned}$$

Decode: Two-stage iterative imputation

- Stage 1: $\mathbf{H}_t^K \rightarrow$ initial predictions.
- Stage 2: Predictions refined on the graph.
- Outputs: $\hat{y}_{t,i}[c]$ at quantiles τ_c for uncertainty estimation.

Imputation Mapping via FibMap

Why a GRNN? Drawing Analogies with Local Physics

The Cable Equation

$$\frac{\partial V}{\partial t} = \nabla \cdot (D \nabla V) - \frac{I_{ion}(V; y)}{C_m}$$
$$\frac{\partial y}{\partial t} = g(V; y)$$

Physical Properties:

1. Neighbouring spatial regions are coupled.
2. Anisotropic diffusion through the $\nabla \cdot (D \nabla V)$ term.
3. Local D and $\frac{I_{ion}}{C_m}$ affect global wave patterns.
4. Threshold-dependent activation and recovery dynamics.

FibMap:

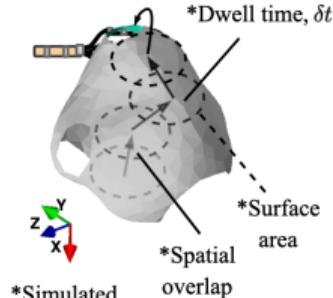
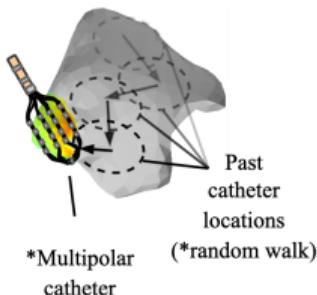
1. Expressed through the graph topology.
2. Anisotropic message passing functions are learnt.
3. Embeddings may capture local parameters.
4. Gated-RNN may capture these non-linear dynamics.

Imputation Mapping via FibMap

Dataset & Training Approach

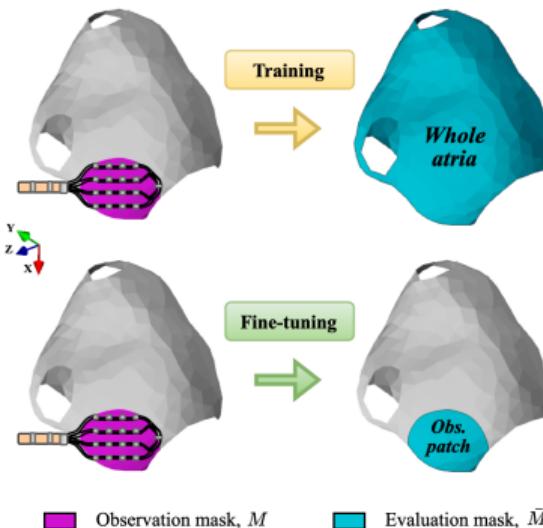
Dataset

- 51 persistent AF patients.
- AcQMap non-contact recordings:
 - Recordings 5-20 seconds per patient;
 - ≈ 3500 nodes, 3000 Hz;
 - Provides real examples of human AF dynamics;
 - Avoids simplified mathematical models.



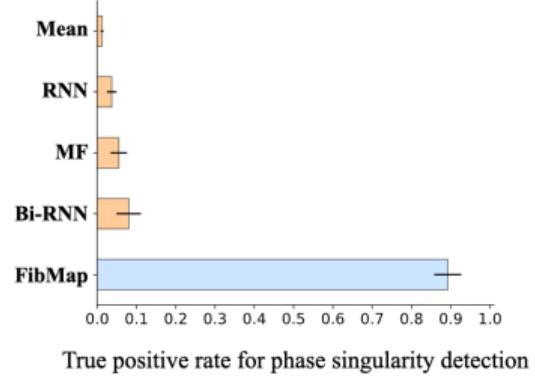
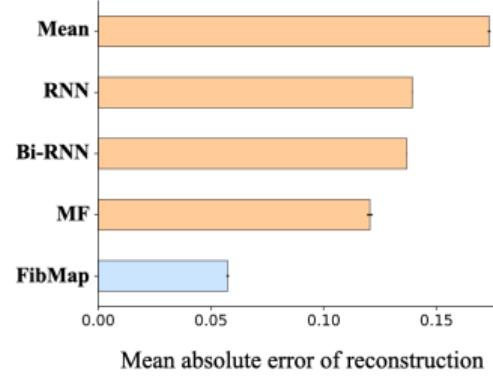
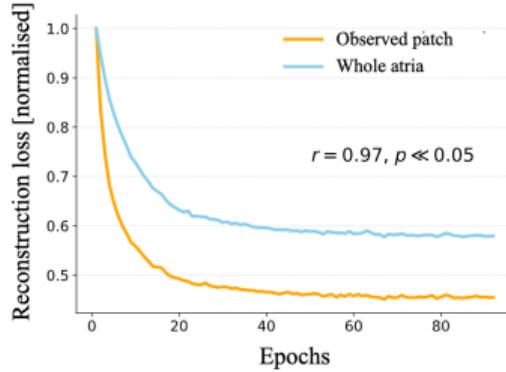
Model Training Strategy

- Self-supervised learning approach: contact mapping is simulated.



Quantitative Results

Reconstruction Performance on Test Patients



Fine-Tuning Validation

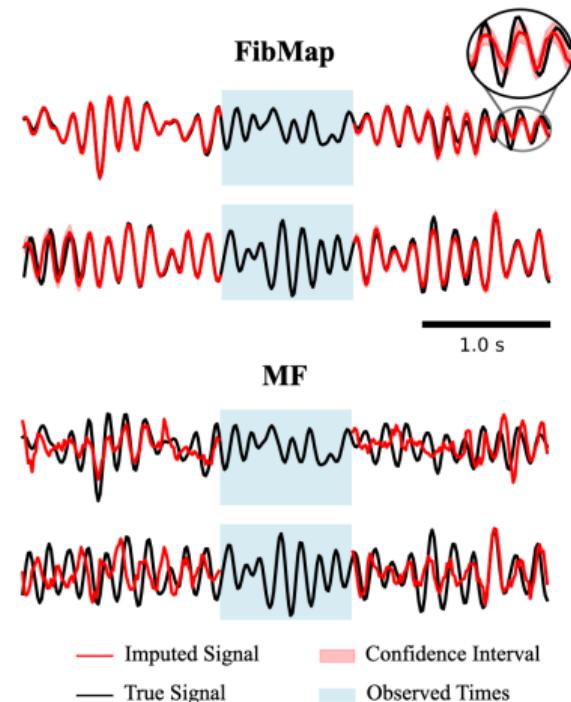
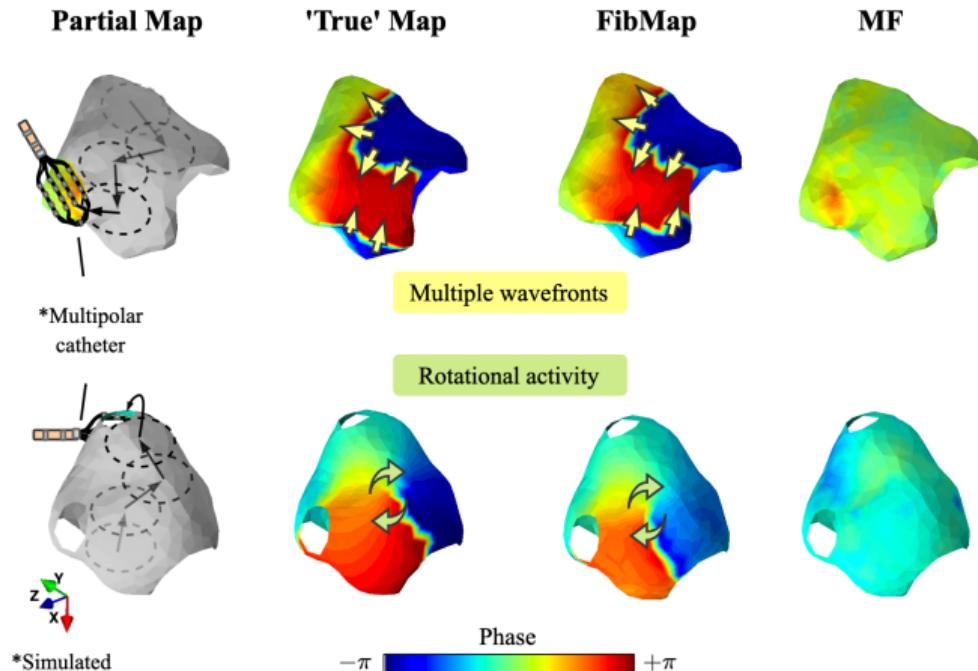
- Strong correlation between observed patch and whole atria losses ($r = 0.97$).
- Enables fast and accurate reconstruction from limited observations (22 mins per patient).

Performance Highlights

- 210% improvement in reconstruction accuracy (MAE) over best baseline.
- 11.1 \times better phase singularity detection (TPR of 89% vs 8%).

Qualitative Results

Visualisation of Imputation Maps

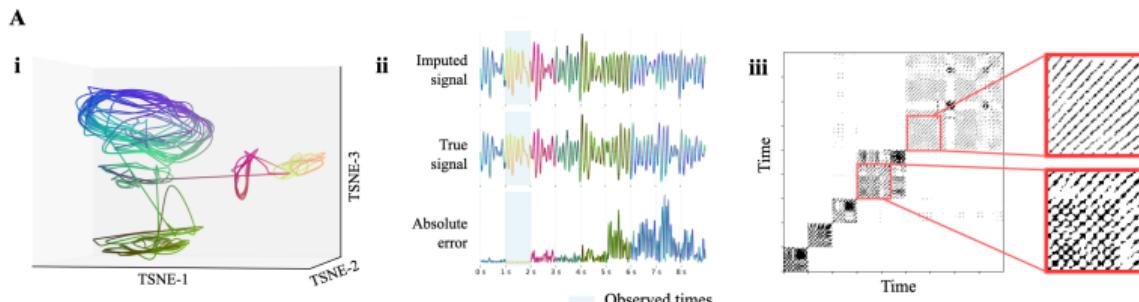


Hidden State and Embedding Analysis

Insights for Electrophenotyping

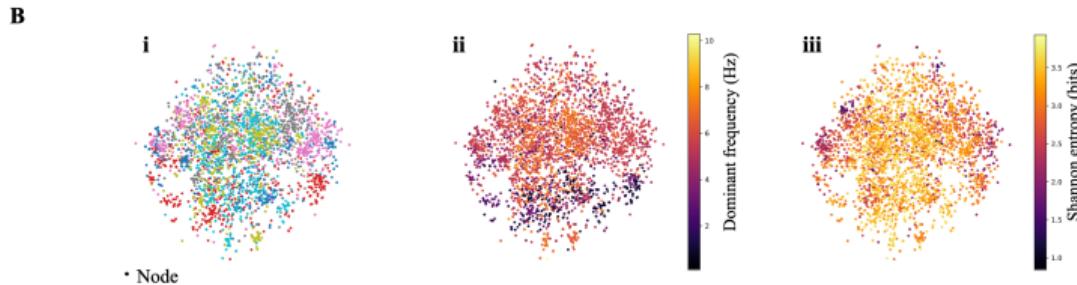
State-Space Dynamics

- Hidden states reveal the chaotic dynamics of AF.
- Orbital patterns around fixed points.
- Recurrence plot reveals structured dynamics.



Embedding Analysis

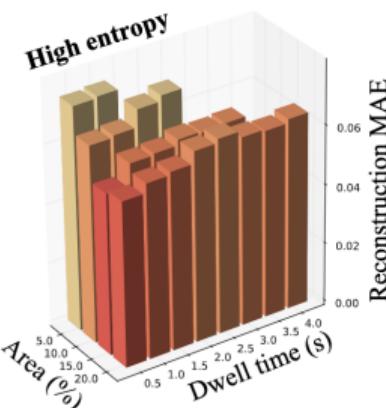
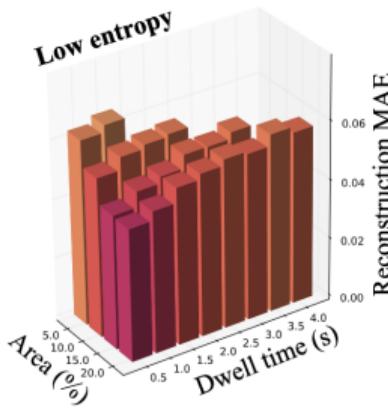
- Node embeddings capture dominant frequency and entropy.
- Potential for AF electrophenotyping.



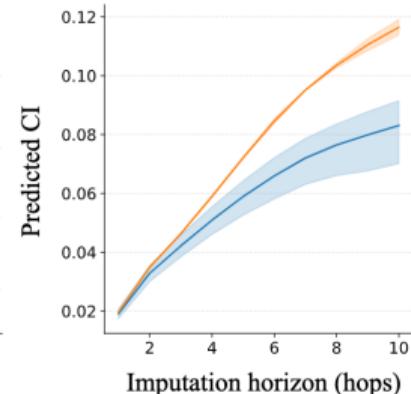
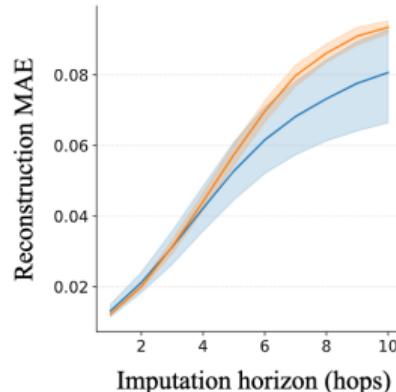
Sensitivity Analysis

Performance with Variations in Sequential Contact Mapping

A



B



— Low entropy — High entropy

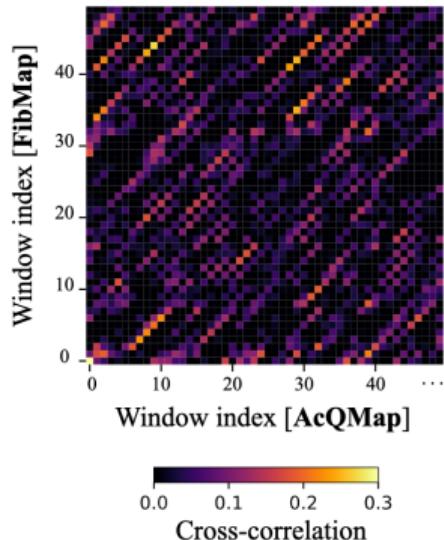
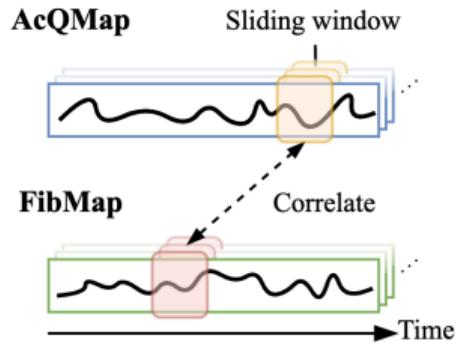
- Prediction accuracy \uparrow as dwell time \downarrow , mapping area \uparrow , and for more organised AF.
- Prediction error and intervals \uparrow as the distance in space and time from valid observations \uparrow .

Clinical Proof-of-Concept

Methodology

Approach

- EnSite Precision HD Grid (contact) vs. AcQMap (ground truth).
- Non-contemporaneous recordings from 3 test set patients.
- Cross-correlation analysis across different time windows.
- Statistical comparison of patient-specific patterns.

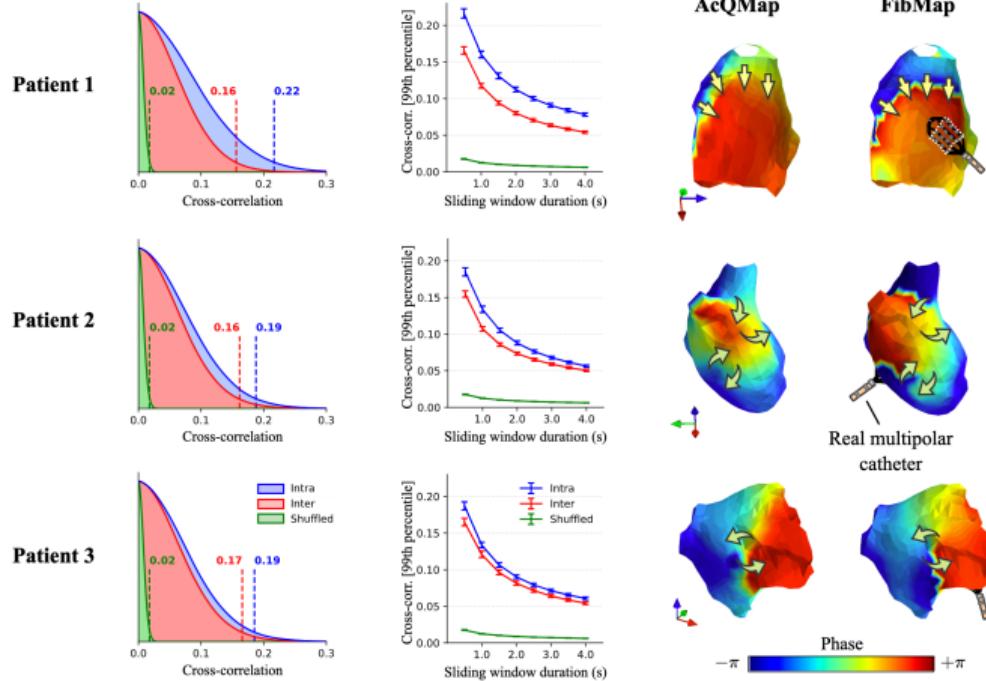


Clinical Proof-of-Concept

Results on Real-World Contact Mapping

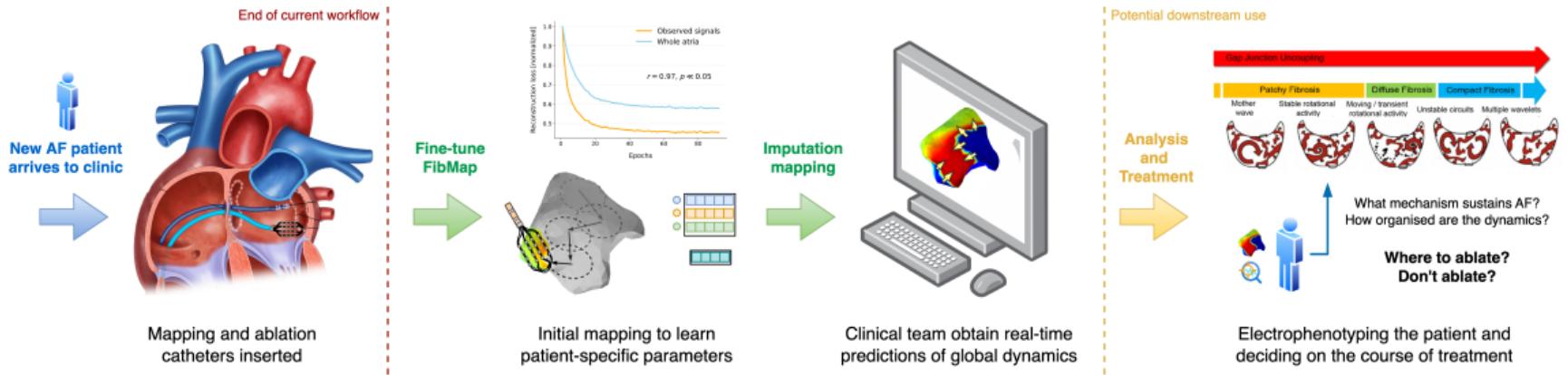
Key Findings

- FibMap captures patient-specific dynamics.
- Significantly higher intra-patient correlations vs. inter-patient.
- Consistent across multiple time scales.
- Reconstructs elements of dynamics not visible in original HD Grid data.
- Demonstrates clinical utility with existing catheters.



Envisioned Clinical Use

Imputation Mapping in Practice



A Path Towards Personalised AF Treatment?

- Imputation mapping predicts global propagation dynamics from sparse measurements.
- Downstream analysis of global maps could enable electrophenotyping of patients and stratification for treatments.
- Moving beyond one-size-fits-all treatment could improve clinical outcomes.

Future Directions

Current Limitations

- Trained on non-contact AcQMap data in the absence of true global ground truth.
- Need to determine optimal spatio-temporal resolution for guiding treatment decisions.

Technical Improvements

- Augment training with high-resolution simulated data to improve resolution if needed.
- Explore hierarchical architectures with virtual nodes for improving long-range imputations.

Clinical Validation

- Validate model's state-space and embedding representations for electrophenotyping.
- Compare with organised arrhythmias (e.g., atrial tachycardia) where sequential mapping can be stitched together.
- Prospective clinical trial: one-size-fits-all vs. imputation-guided personalised ablation strategies.

Summary and Conclusions

FibMap: Key Contributions

- Novel imputation mapping approach for AF.
- 210% improvement over baseline methods.
- 11× better phase singularity detection.
- Fast adaptation to new patients (22 min).
- Uncertainty estimation to guide interpretation.
- Real-world proof-of-concept with clinical data.
- Interpretable patient embeddings and model state-spaces.

Clinical Impact

- Integrates seamlessly with existing clinical catheters and workflows.
- Reveals AF mechanisms not visible with conventional mapping.
- Potential to reduce procedure time, complexity, and risk.
- Pathway to personalised AF treatment beyond one-size-fits-all approaches.

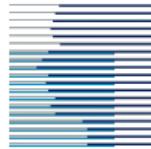
Acknowledgements

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Thank you. Questions?



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