# Upper-Limb Pose Prediction using Six-Axis Wrist-Worn IMUs

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## **Motivation**

- Growing demand for wearable-based human pose estimation
- Wrist-worn IMUs are lightweight, affordable, and practical
- Challenge: Inferring full arm motion from limited IMU input
- Goal: Predict upper-limb skeletal motion using only 6-axis wrist IMU

## **Project Overview**

- Predict 3D joint coordinates from wrist-worn IMU data
- Inputs: Accelerometer + Gyroscope (6-axis)

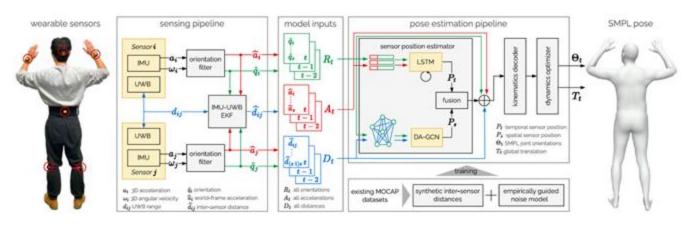
Sensor Type	Axis X	Axis Y	Axis Z
Accelerometer	ax	ay	az
Gyroscope	gx	gy	gz

- Outputs: 3D skeletal positions of upper limb
  - Shoulder, Elbow, Wrist, Finger (Left/Right)
- Evaluation: Compare predicted vs ground-truth MoCap positions



## Related works

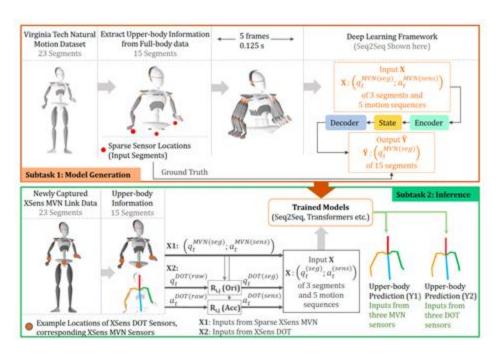
Ultra Inertial Poser: Scalable Motion Capture and Tracking from Sparse IMU and UWB



- This paper uses **sparse IMU + UWB sensors** to predict **full-body pose**.
- Our project is different: we use only two wrist-worn IMUs to predict only the upper-limb pose.
- Takeway: They showed that even with sparse sensors, accurate pose prediction is possible by using graph-based fusion of signals. -> We can apply temporal sequence models (LSTM) to capture motion over time.

## Related works

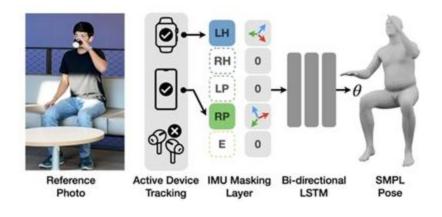
Capturing Upper Body Kinematics and Localization with Low-Cost Wearable Sensors



- This paper uses three IMUs (wrists + pelvis) to predict upper-body kinematics.
- Our project is even more challenging: two wrist IMU, no pelvis sensor.
- Takeaway: Their use of a Seq2Seq deep learning model showed that even sparse IMUs can predict upper-limb motion well. -> We again saw the importance of temporal sequence modeling with LSTM and similar models

## Related works

IMUPoser: Full-Body Pose Estimation using IMUs in Phones, Watches, and Earbuds



- IMUPoser demonstrates **real-time full-body pose estimation** from only consumer IMUs (phones, watches, earbuds) using **a two-layer bi-LSTM** and a brief inverse-kinematics (**IK**) refinement.
- IMUPoser relies on sensor-provided **global orientations** with an **LSTM+IK pipeline** and active device-tracking, while our approach sensor data in **local orientations**, then uses a **Bi-LSTM** for end-to-end pose regression with **biomechanical constraints**.

## **Project Objectives**

#### Goal:

Apply and experiment with methodologies learned in class to predict upper-limb skeletal motion using only wrist-worn 6-axis IMUs.

#### **Key Investigation Points:**

- What types of models (e.g., LSTM, BiLSTM) best capture upper-limb motion from IMU data?
- How much impact does IMU preprocessing (e.g., filtering, orientation estimation) have on model performance?
- Can introducing biomechanical constraints improve an accuracy of predicted poses?

## **Dataset**

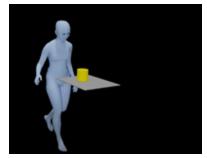
AMASS: 300 subjects, 40+ hours of motion capture

GRAB: Subset of AMASS. Detailed hand-object interaction dataset

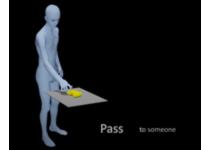
- 10 subjects interact with 51 everyday objects
- Activities: Lift, pass, off-hand pass, and use

#### Data details:

- Inertial Data (Accel, gyro): Two IMUs, which each is located on a forearm
- MoCap: shoulders, elbows, wrists, and thumbs



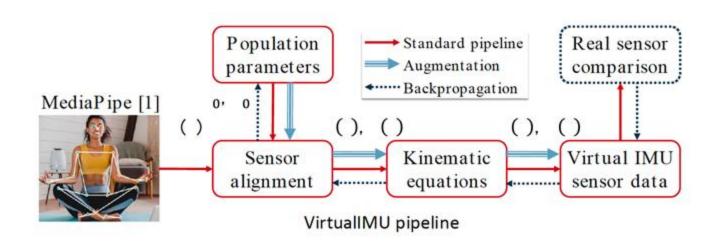






## **IMU** Data Generation

- Use Virtual IMU to synthesize IMU data from MoCap
- Bypassed MediaPipe (red path in pipeline)
- Backprop-based sensor alignment (optional)



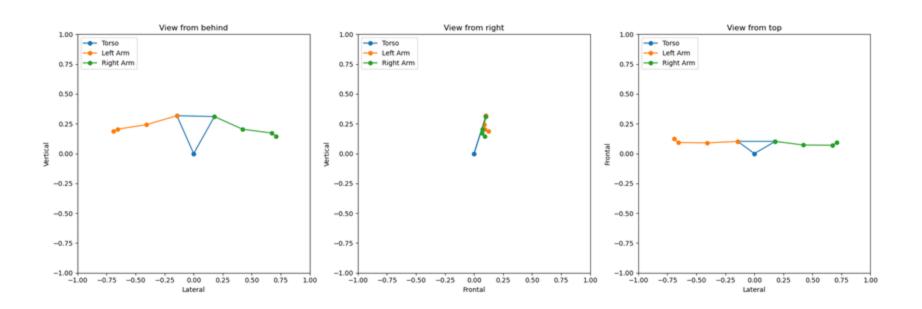
## Data preprocessing

- Filtering:
  - Reduce high-level noises and drift in IMU acceleration and gyroscope data
  - Using low-pass and band-pass filters (0.1 20 Hz)
- Estimate sensor orientation and transform acceleration and angular velocity into the global coordinate system (Task 2.6 Assignment 1)
  - o Steps:
    - Estimate orientation using AQUA algorithm.
    - Rotate local IMU data to global coordinates.
    - Remove gravity from the Z-axis.
- Data Segmentation:
  - Sliding window approach with window size of 1 second and overlap of 75%

## Example

Ground-truth Pose (MoCap)

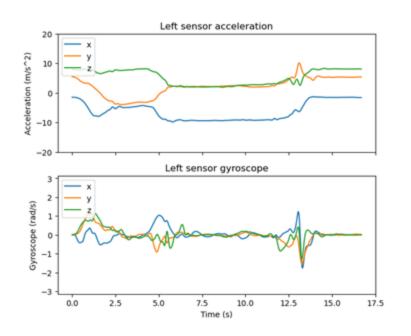
• Directly from GRAB dataset

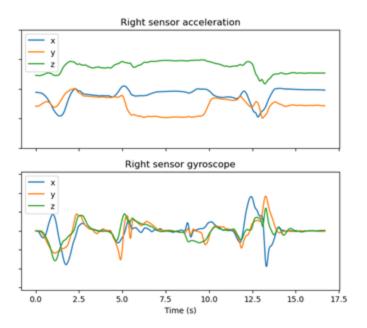


## Example

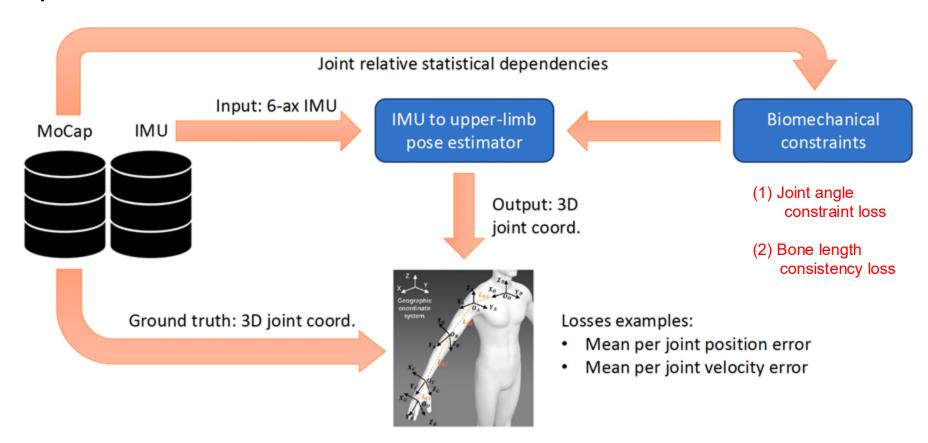
Input IMU (Sensor data)

Generated from GRAB Mocap via Virtual-IMU





## **Pipeline**



## Biomechanical constraints

Vetrice, Georgiana & Deaconescu, Andrea. (2017). Development of elbow rehabilitation equipment using pneumatic muscles. MATEC Web of Conferences

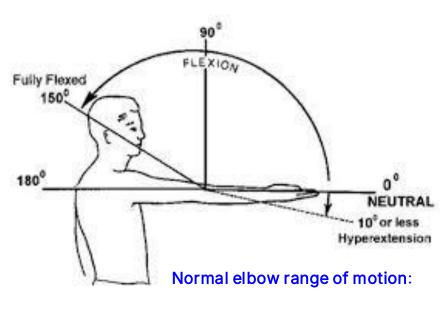
## (1) Joint angle constraint loss

#### What does it check?

 elbow joint flexion angle — the angle formed at the elbow between the upper arm and forearm

#### How is it calculated?

- Use shoulder → elbow → wrist to compute the joint angle
- Apply penalty if angle is outside the valid range
- Average penalties across batch and time steps



Full extension: ~0°

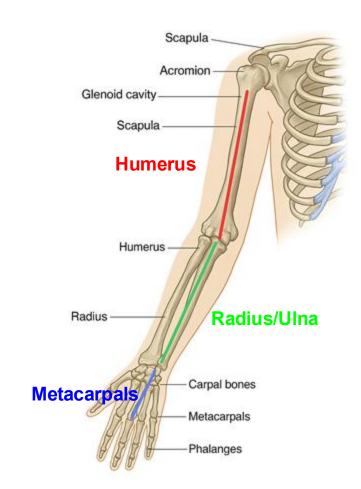
Full flexion: ~150°

## Biomechanical constraints

- (2) Bone length consistency loss
  - What does it check?
    - lengths of the bones

### ?How is it calculated?

- For each bone, the length is computed using the formula length = sqrt(sum(vector^2))
- Measure variance over time
- Apply separately to upper arm, forearm, and hand, for both the left and right arms
- Average all variances as the final loss



## Biomechanical constraints

### (1) Joint angle constraint loss

- Joint-Angle Coordination Patterns Ensure
   Stabilization of a Body-Tool System (2016,
   Frontiers in Psychology, Van der Steen et al)
- 3D human pose estimation based on 2D–3D consistency with synchronized adversarial training (2024, Robotics and Autonomous Systems, Yicheng Deng et al)
- Human Joint Angle Estimation Using Deep Learning-Based Three-Dimensional Human Pose Estimation for Application in a Real Environment (2024, MDPI, Jin-Young Choi et al)

### (2) Bone length consistency loss

- Motion Projection Consistency Based 3D
   Human Pose Estimation with Virtual Bones
   from Monocular Videos (2022, IEEE
   transaction on cognitive and developmental
   systems, Guangming Wang et al)
- A Geometry Loss Combination for 3D Human Pose Estimation (2024 IEEE/CVF Winter Conference on Applications of Computer Vision (WACV), Ai Matsune et al)
- BLAPose: Enhancing 3D Human Pose
   Estimation with Bone Length Adjustment
   (2024, Chih-Hsiang Hsu et al, 2024)

## **Loss Functions**

Without biomedical constraints:

$$Loss = MSE$$

With biomedical constraints:

$$Loss = \lambda_1 MSE + \lambda_2 Loss_{angle} + \lambda_3 Loss_{bone}$$

MSE: Mean Square Error

 $Loss_{angle}$ : Joint angle constraint loss  $Loss_{bone}$ : Bone length consistency loss

 $\lambda_1, \lambda_2, \lambda_3$ : Weights

## Model Architectures

#### LSTM (Baseline)

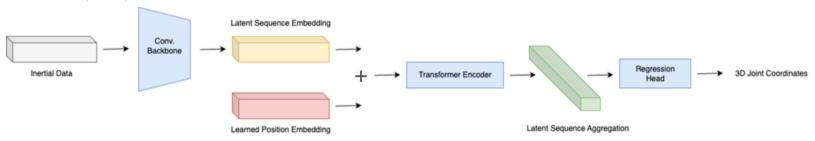
- 2-layer, unidirectional
- Models short-range dynamics with low latency and modest compute

#### **Bidirectional LSTM**

- 2-layer, processes sequences forward + backward
- Captures both past and future temporal dependencies

#### ConvTransformer

- Inspired by Shavit and Klein's 2021 work [1]
- Combines convolutional feature extraction with a Transformer encoder to model spatial-temporal patterns for 3D joint prediction



[1] Shavit, Y., & Klein, I. (2021). Boosting inertial-based human activity recognition with transformers. *IEEE Access*, 9, 53540-53547.

## **Evaluation Metrics**

We evaluate the model using quantitative metrics:

#### Mean Per Joint Position Error (MPJPE):

- Measures the average Euclidean distance between predicted and ground truth joint positions.
- Lower MPJPE indicates higher pose accuracy.

$$MPJPE = rac{1}{N_F} \cdot rac{1}{N_J} \sum_{f,j} \left\lVert p_{f,j} - \hat{p}_{f,j} 
ight
Vert_2$$

#### Where:

- ullet  $N_F$  is the number of frames
- $N_J$  is the number of joints
- ullet  $p_{f,j}$  is the ground truth position of joint j at frame f
- $\hat{p}_{f,i}$  is the predicted position

## **Evaluation Metrics**

We evaluate the model using quantitative metrics:

#### Mean Per Joint Velocity Error (MPJVE):

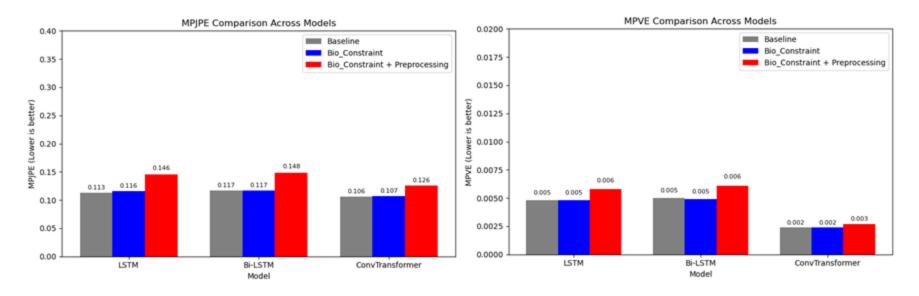
- Measures the average difference in joint velocities between predicted and ground truth over time.
- Captures temporal smoothness and motion consistency.

$$MPJVE = rac{1}{N_F} \cdot rac{1}{N_J} \sum_{f,j} \left\| v_{f,j} - \hat{v}_{f,j} 
ight\|_2$$

#### Where:

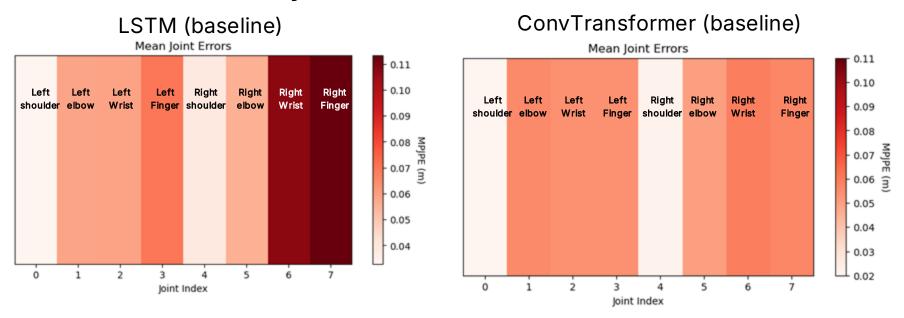
- $N_F$  is the number of frames
- N<sub>J</sub> is the number of joints
- ullet  $v_{f,j}$  is the ground truth velocity of joint j at frame f
- $\hat{v}_{f,j}$  is the predicted velocity

## Result



- ConvTransformer (baseline) delivers the best overall performance.
- **LSTM** shows the most significant performance degradation under the *Bio Constraint + Preprocessing* condition, followed by **Bi-LSTM**.
- ConvTransformer stayed stable and robust across all experiments.

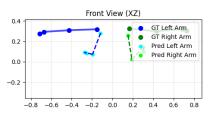
## Joint-wise difficulty

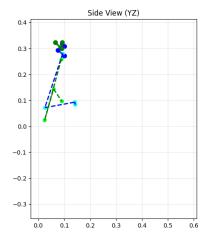


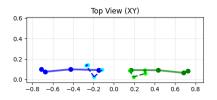
- Overall error drop: ConvTransformer roughly halves the worst-case errors (joints 6 & 7) and reduces average MPJPE across all joints.
- Variance shrinks: LSTM errors span ~0.03–0.115 m, whereas ConvTransformer compresses that range to ~0.02–0.057 m.

## Drinking water

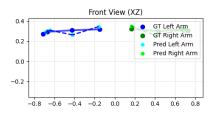
## LSTM (Baseline)

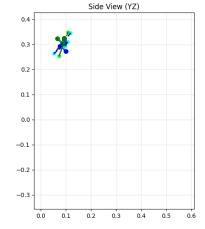


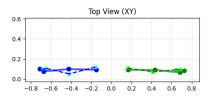




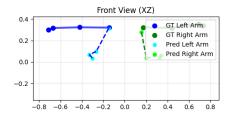
## ConvTransformer (with bioconstraint)



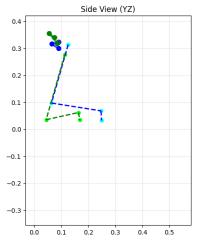


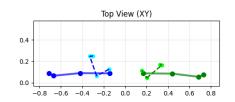


## LSTM (Baseline)

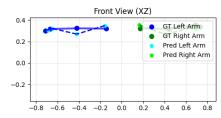


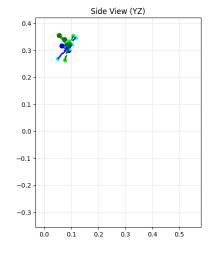
### Peel with a knife

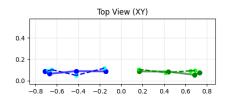




## ConvTransformer (with bioconstraint)

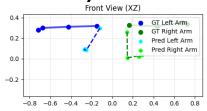


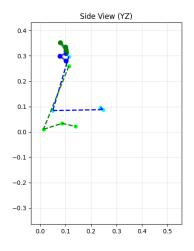


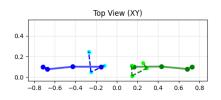


## Picking up a cup

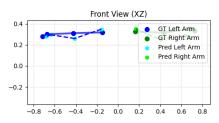
## LSTM (Baseline)

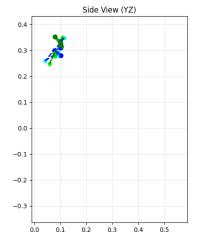


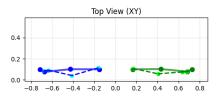




## ConvTransformer (with bioconstraint)







## Conclusion

- Model-Wise Performance Insights:
  - LSTM and ConvTransformer showed the best overall performance, achieving the lowest MPJPE and MPVE under the baseline (no constraint) condition.
  - The LSTM delivers nearly transformer-level accuracy with fewer parameters and much lower inference latency, making it the optimal choice for resource-constrained, real-time deployment.
- Preprocessing steps mostly degraded performance, likely due to information loss, or sensitivity to transformed inputs.

## Future work

- Domain gap between synthetic IMU and real IMU / Real-world testing with actual IMU
- Hyperparameter tuning
- Extending Joint Constraints to Multi-Axial Joints

## Thank you!