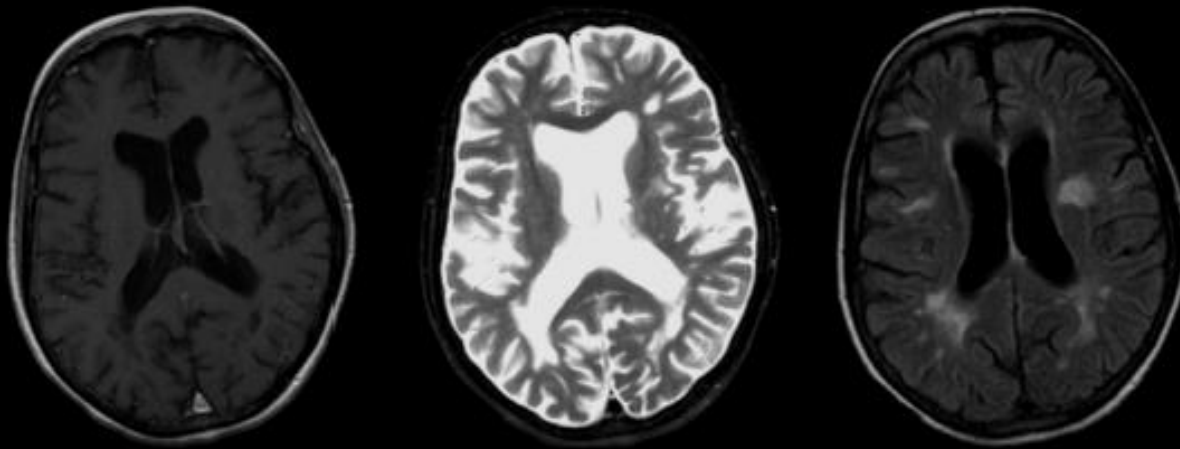


# MRI:

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T<sub>1</sub> vs. T<sub>2</sub> Weighting  
Spin Echo  
Gradient Echo  
Inversion Recovery



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ENGG 4040  
Medical Imaging Modalities

# Overview

## Review:

- Resonance
- $T_1$  &  $T_2$
- Spatial Encoding

## Spin Echo

- Sequence
- Equation

## $T_1$ and $T_2$ Weighting

## Gradient Echo

- Sequence
- Equation

## Inversion Recovery

- Sequence
- Equation

## Summary

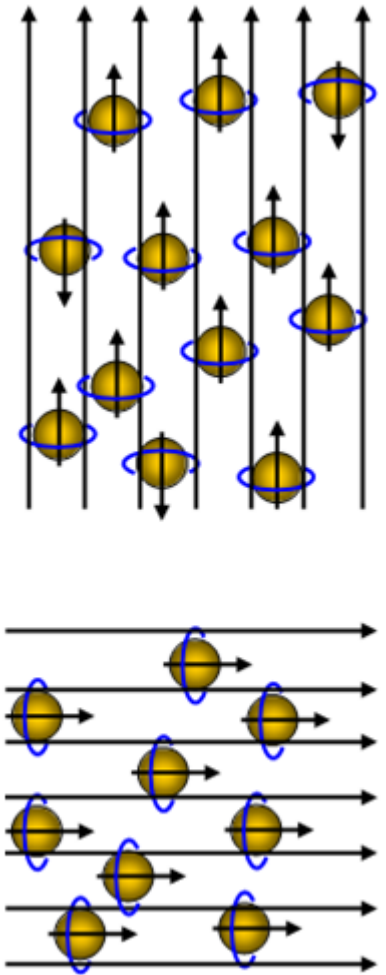
# Review: Resonance

## Magnetic Field

- Atoms spinning & precessing due to  $B_o$
- Precession  $f_L$  proportional to  $B$

## Transverse RF Pulse

- $90^\circ$  RF\* pulse “knocks” spin axes down  
\*(rotating frame of reference)
- Creates net moment  $M$  in rotating  $XY$  plane

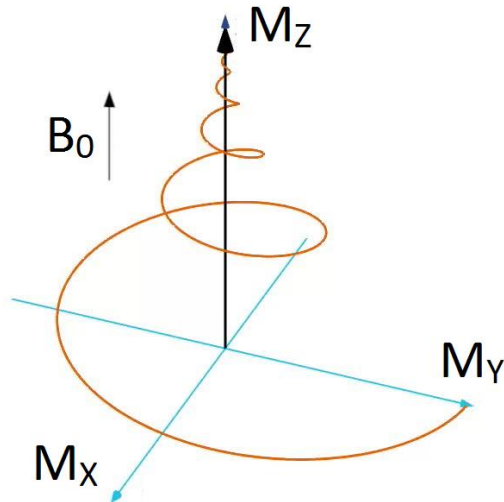


# Review: $T_1$ and $T_2$

## $T_1$

- Rate of recovery of moment in  $B_0$  direction:  $M_Z$
- “Spin-Lattice”

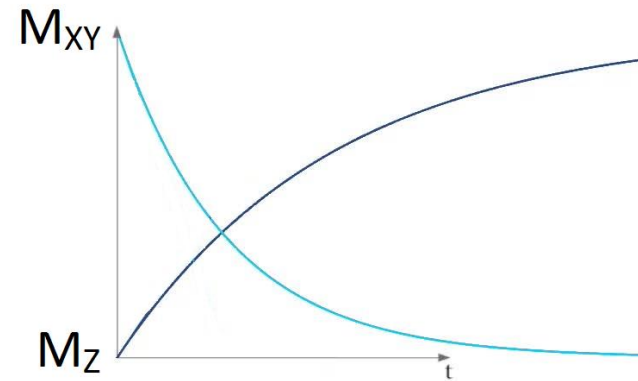
$$M_Z = M_0 \left( 1 - e^{-\left(\frac{t}{T_1}\right)} \right)$$



## $T_2$

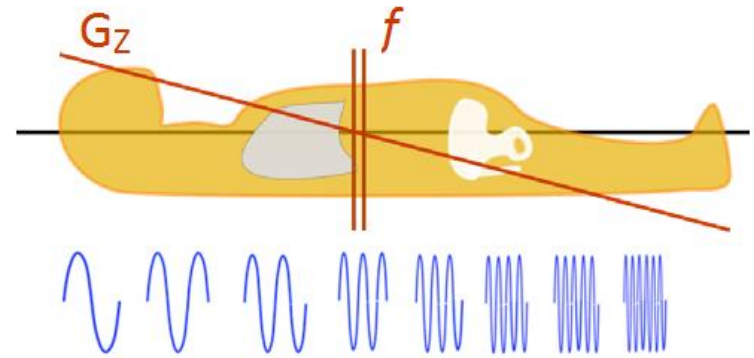
- Rate of decay of moment in  $B_1$  direction:  $M_{XY}$
- “Spin-Spin”

$$M_{XY} = M_0 \left( e^{-\left(\frac{t}{T_2}\right)} \right)$$



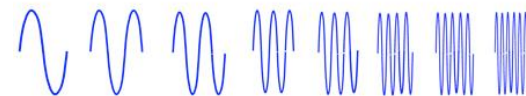
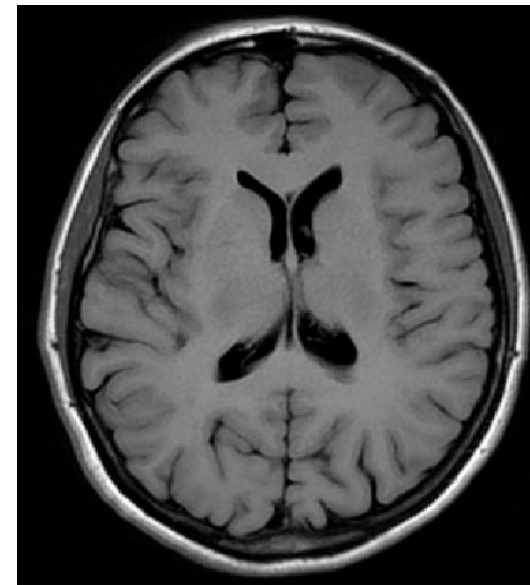
# Review: Spatial Encoding

1. Slice Select: During RF *only excite one plane*



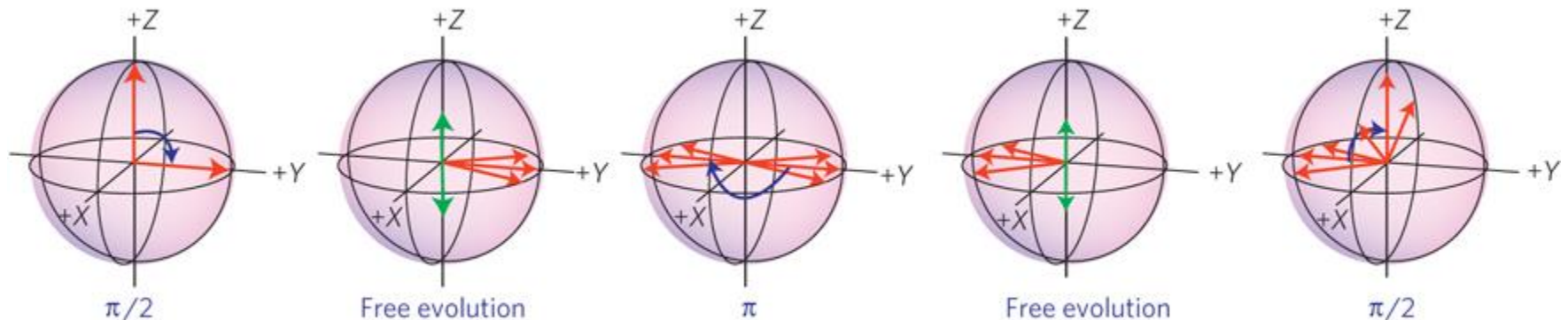
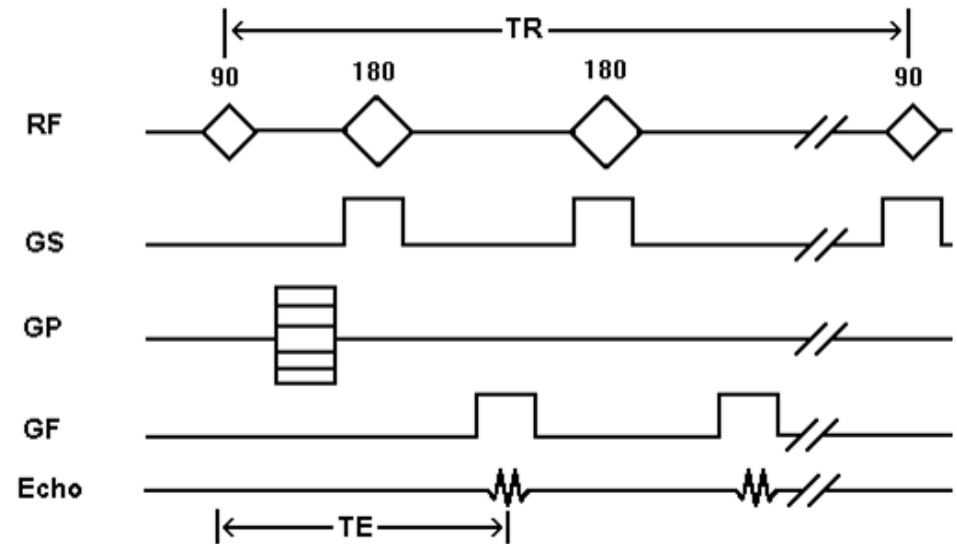
2. Frequency Encode: *frequency varies across plane*

3. Phase Encode: *phase varies across plane in other direction*



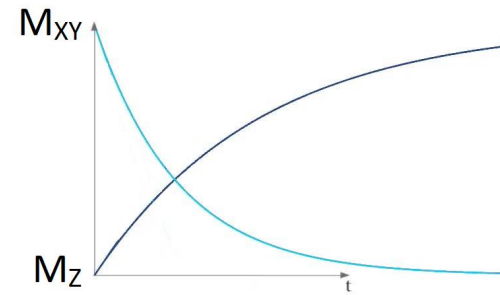
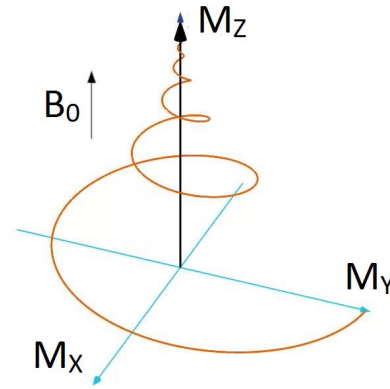
# Spin Echo Sequence

- Refocus  $M_{XY}$  using  $180^\circ$
- Multiple  $180^\circ$  pulses:  
Multiple echoes  
... Faster Acquisition



# Spin Echo Equation (Signal Magnitude)

$$\Psi_{SE} = \Psi_0 e^{-\left(\frac{TE}{T2}\right)} \left(1 - e^{-\left(\frac{TR}{T1}\right)}\right)$$



## $T_1$ & TR

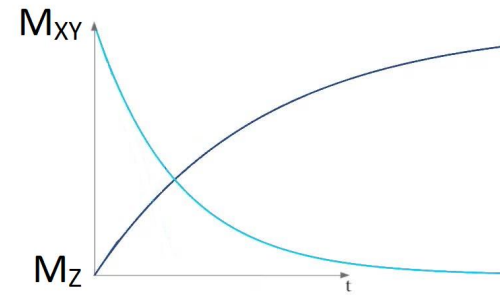
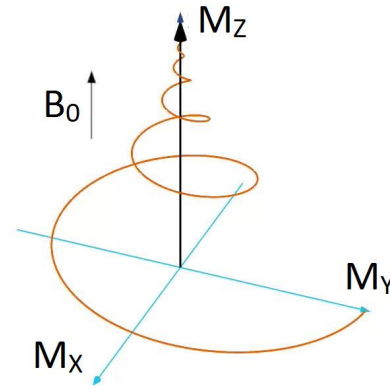
- Long TR: more  $M_z$  recovered for next excitation
- Amount of  $M_z$  recovered depends on tissue  $T_1$

## $T_2$ & TE

- Very long TE: signal strength ( $M_{xy}$ ) decays too much
- Very short TE: tissue  $T_2$  has minimal impact

# $T_1$ and $T_2$ Weighting

$$\Psi_{SE} = \Psi_0 e^{-\left(\frac{TE}{T_2}\right)} \left(1 - e^{-\left(\frac{TR}{T_1}\right)}\right)$$



## $T_1$ -Weighting

- $T_1 \approx TR$  → Emphasize differences in  $M_z$  recovery
- Short TE → Minimize impact of  $T_2$

## $T_2$ -Weighting

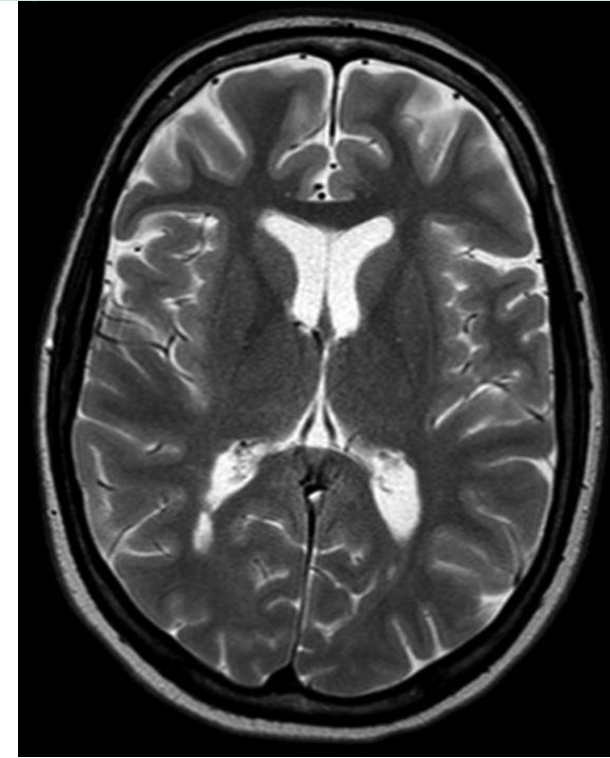
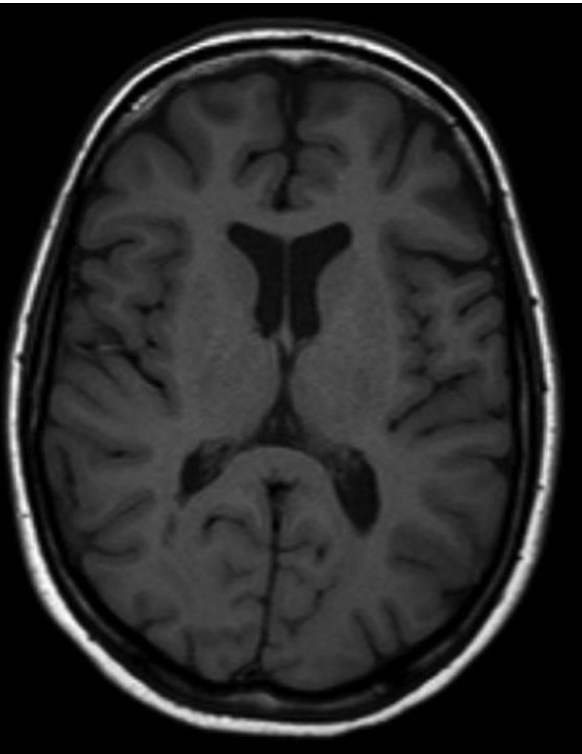
- $T_2 \approx TE$  → Maximize contrast of  $T_2$
- Long TR → Allow full  $M_z$  recovery



# T<sub>1</sub> and T<sub>2</sub> Weighting

## T<sub>1</sub>-Weighting

- Bright: short T<sub>1</sub>
  - Dark: long T<sub>1</sub>
- $$\left. \begin{array}{l} \text{Bright: short } T_1 \\ \text{Dark: long } T_1 \end{array} \right\} \Psi_{SE,T_1} \approx \Psi_0 \left( 1 - e^{-\left(\frac{TR}{T_1}\right)} \right)$$



## T<sub>2</sub>-Weighting

- Bright: long T<sub>2</sub>
  - Dark: short T<sub>2</sub>
- $$\Psi_{SE,T_2} \approx \Psi_0 e^{-\left(\frac{TE}{T_2}\right)} \left\{ \begin{array}{l} \text{Bright: long } T_2 \\ \text{Dark: short } T_2 \end{array} \right.$$

# Summary: Spin Echo Weighting

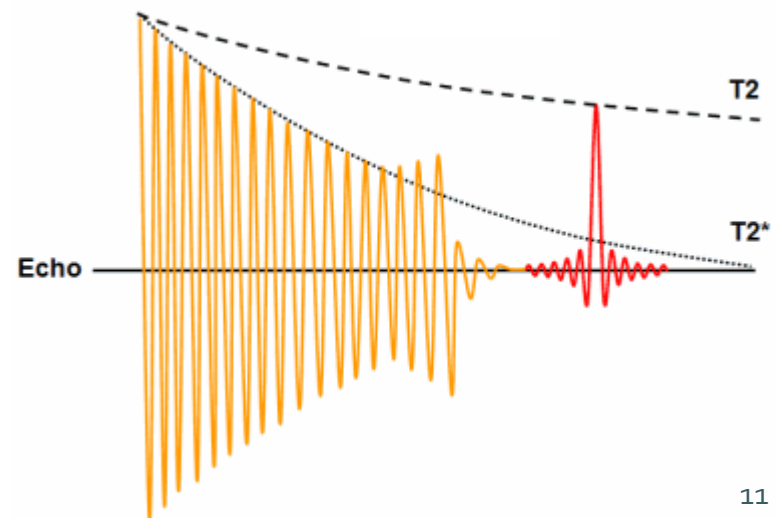
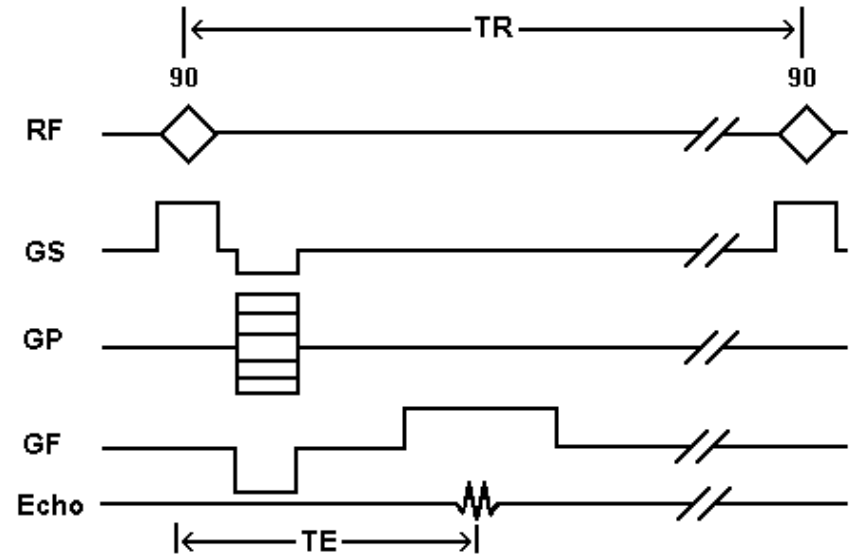
$$\Psi_{SE} = \Psi_0 e^{-\left(\frac{TE}{T2}\right)} \left(1 - e^{-\left(\frac{TR}{T1}\right)}\right)$$

$$\{T1, T2\} \sim (x, y)$$



# Gradient Echo Sequence

- Another way to refocus  $M_{XY}$ :  
use spatial gradients to de/re-phase spins
- $-0.5 \text{ Gf}$  during phase encode  
 $+1.0 \text{ Gf}$  during readout
- Again, multiple gradients:  
Multiple echoes: "Fast GE"  
... Faster Acquisition



# Gradient Echo Equation

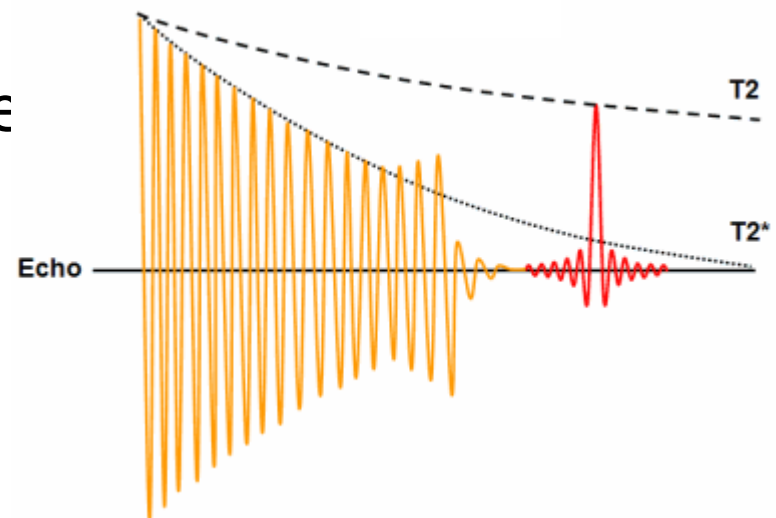
$$\Psi_{GE} = \Psi_0 e^{-\left(\frac{TE}{T2^*}\right)} \left(1 - e^{-\left(\frac{TR}{T1}\right)}\right) \left(\frac{\sin \theta}{1 - \cos \theta \cdot e^{-\left(\frac{T1}{TR}\right)}}\right)$$

Why  $\theta \neq 90^\circ$ ?

- We don't need  $180^\circ$  to act on  $XY$  plane!
- Faster!

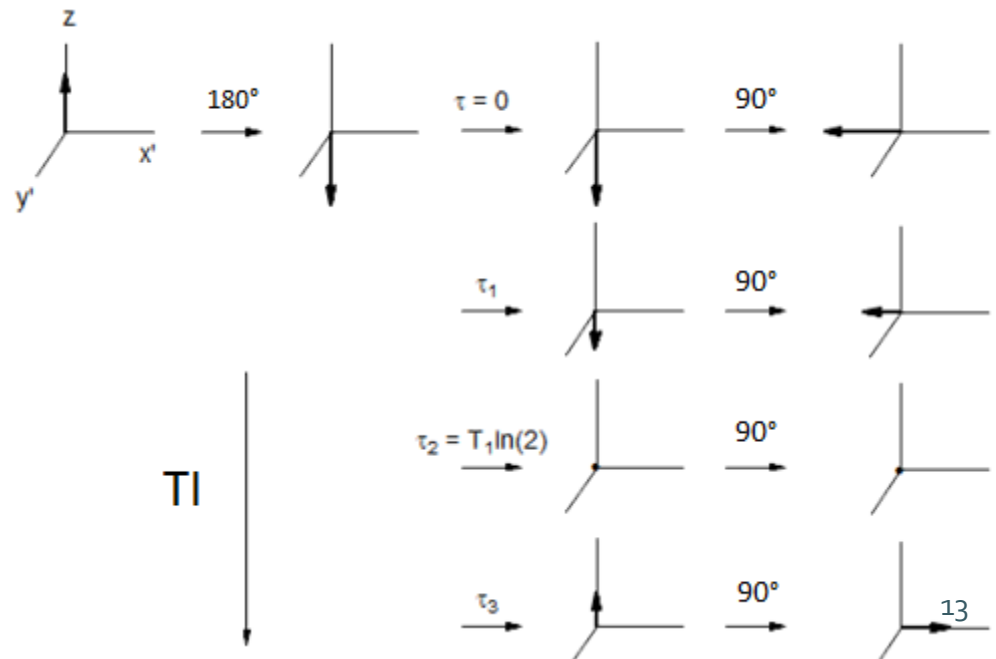
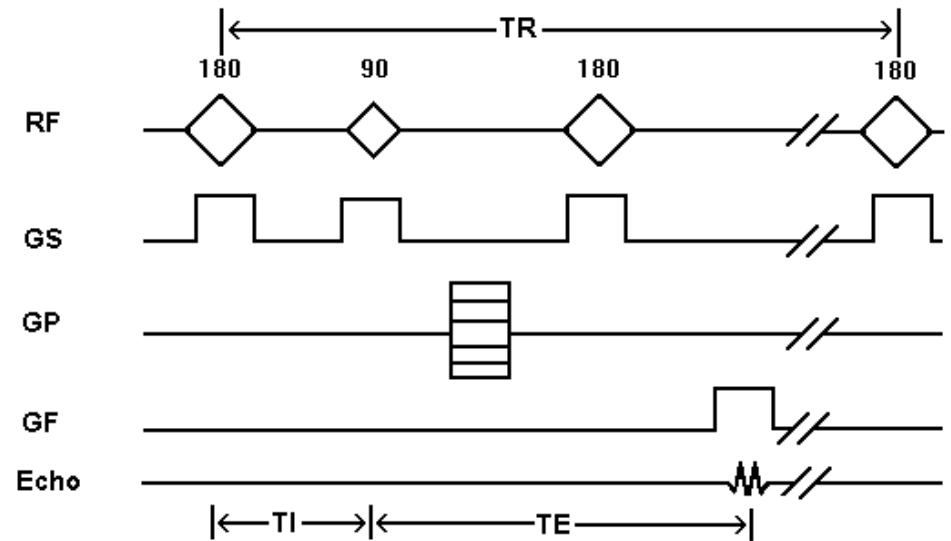
...Need not wait for  $M_z$  recove

- What if  $\theta = 90^\circ$ ?



# Inversion Recovery Sequence

- Want to null the signal from a tissue "K".
- Apply  $180^\circ$  before  $90^\circ$  pulse so  $M_{Z"K"}$  is zero when we apply  $90^\circ$
- Multiple echoes?  
*Nope...*



# Inversion Recovery Equation

$$\Psi_{\text{IR}} = \Psi_0 e^{-\left(\frac{TE}{T2}\right)} \left( 1 + e^{-\left(\frac{TR}{T1}\right)} - 2e^{-\left(\frac{TI}{T1}\right)} \right)$$

## Selecting TI

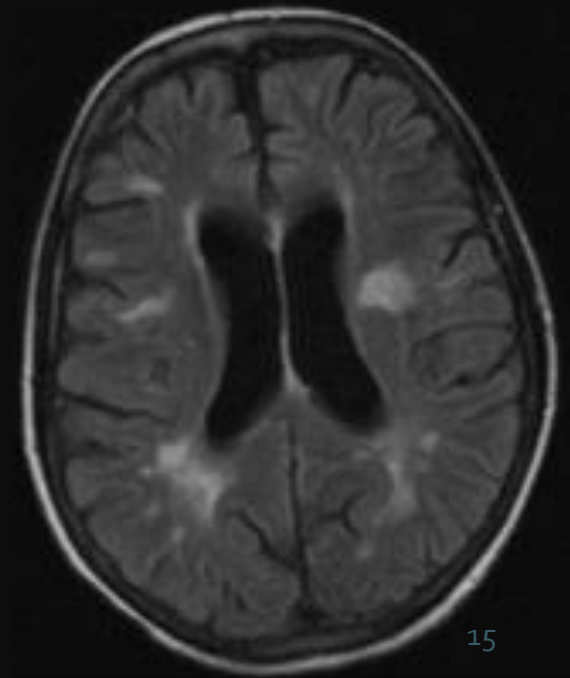
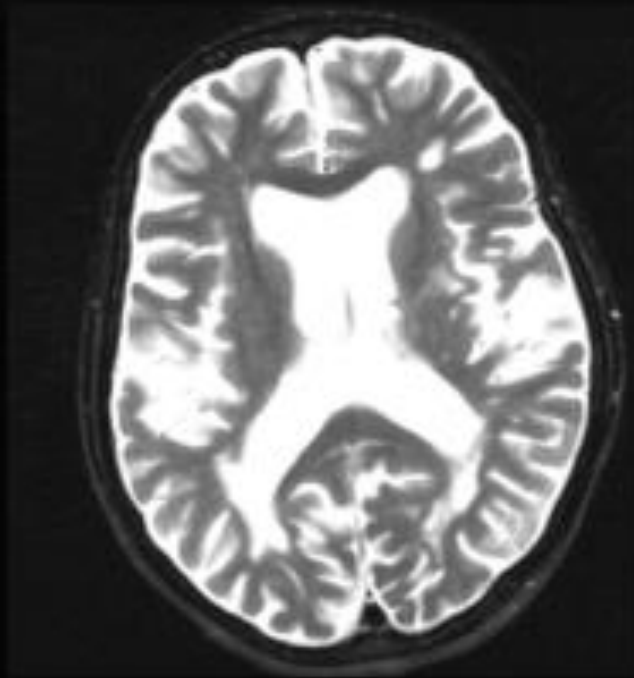
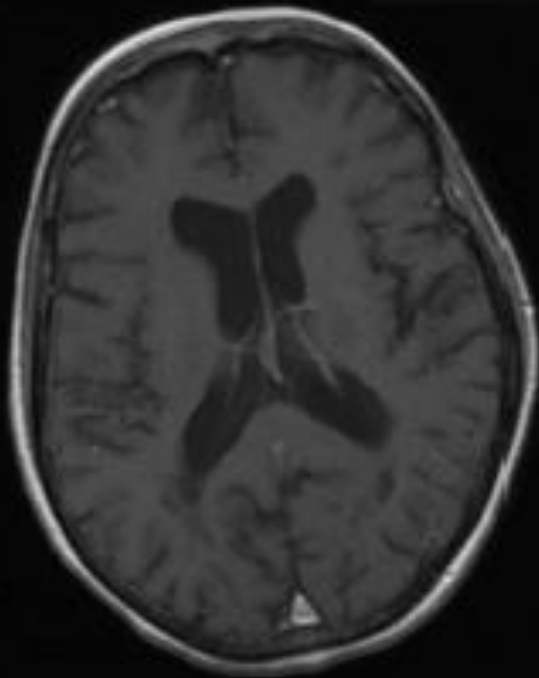
- Not simply  $(1/2) T1_K$ : these are exponential decays!

$$TI = \ln(2) \cdot T1_K$$

- Can null signal from any tissue!
- However: tissues with similar  $T1$  will be affected
- Typically, IR sequences are  $T2$ -weighted, e.g. FLAIR

# Case Study: White Matter Lesions

- Lesions of MS; correlated with Alzheimer's, stroke risk
- T<sub>1</sub>: no contrast
- T<sub>2</sub>: bright, but periventricular uncertainty...
- **FLAIR**: just right!



# Summary: SE ( $T_1$ & $T_2$ ) vs. GE vs. IR

$$\Psi_{SE} = \Psi_0 e^{-\left(\frac{TE}{T_2}\right)} \left(1 - e^{-\left(\frac{TR}{T_1}\right)}\right)$$

180° flip → rephase

$$\Psi_{SE,T_1} \approx \Psi_0 \left(1 - e^{-\left(\frac{TR}{T_1}\right)}\right)$$

Bright: short  $T_1$

$$\Psi_{SE,T_2} \approx \Psi_0 e^{-\left(\frac{TE}{T_2}\right)}$$

Bright: long  $T_2$

$$\Psi_{GE} = \Psi_0 e^{-\left(\frac{TE}{T_2^*}\right)} \left(1 - e^{-\left(\frac{TR}{T_1}\right)}\right) \left(\frac{\sin \theta}{1 - \cos \theta \cdot e^{-\left(\frac{TR}{T_1}\right)}}\right)$$

Gradients → rephase

$$\Psi_{IR} = \Psi_0 e^{-\left(\frac{TE}{T_2}\right)} \left(1 + e^{-\left(\frac{TR}{T_1}\right)} - 2e^{-\left(\frac{TI}{T_1}\right)}\right)$$

Null specific tissue