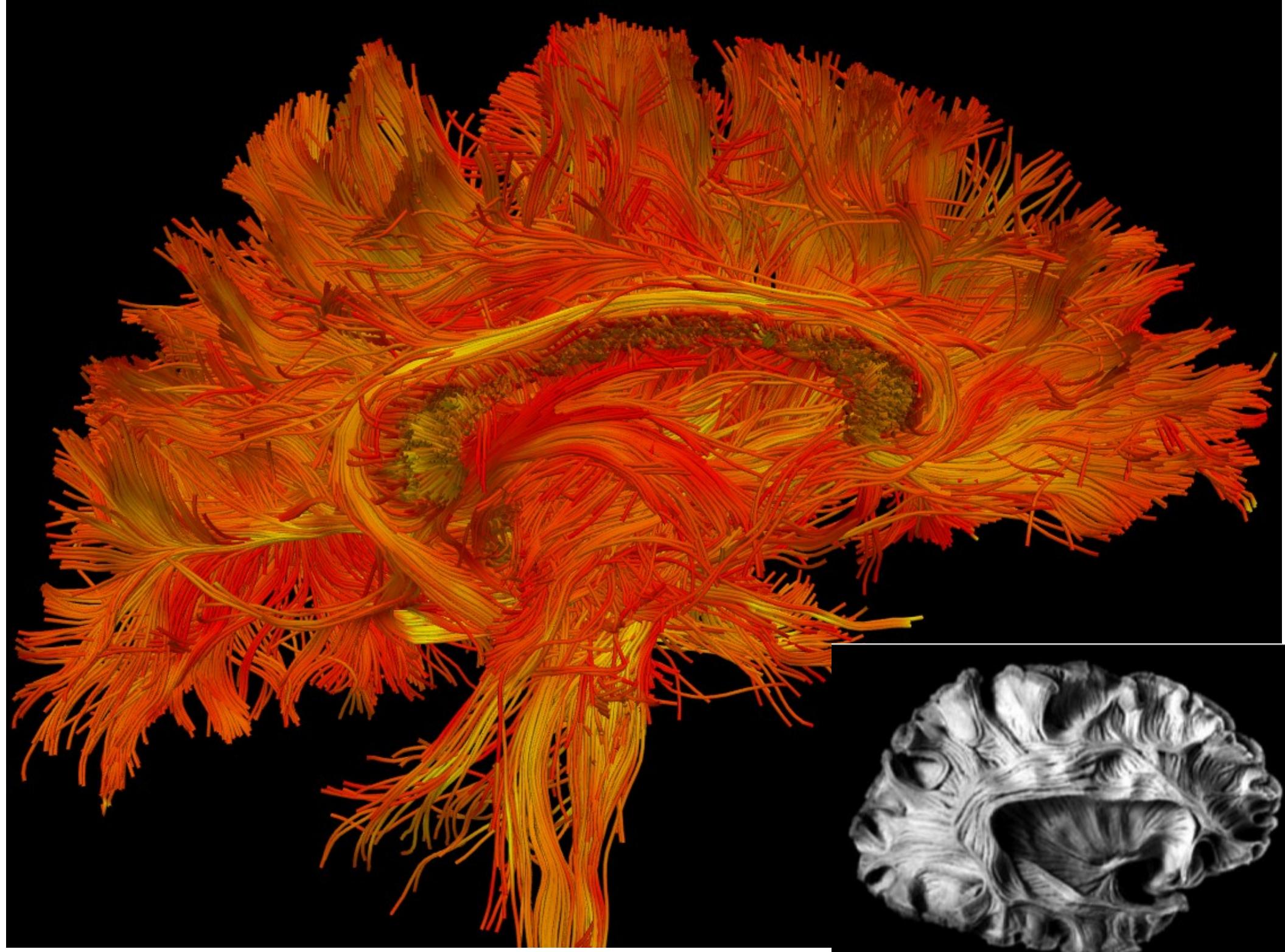


Neural Tractography Using an Unscented Kalman Filter

James Malcolm

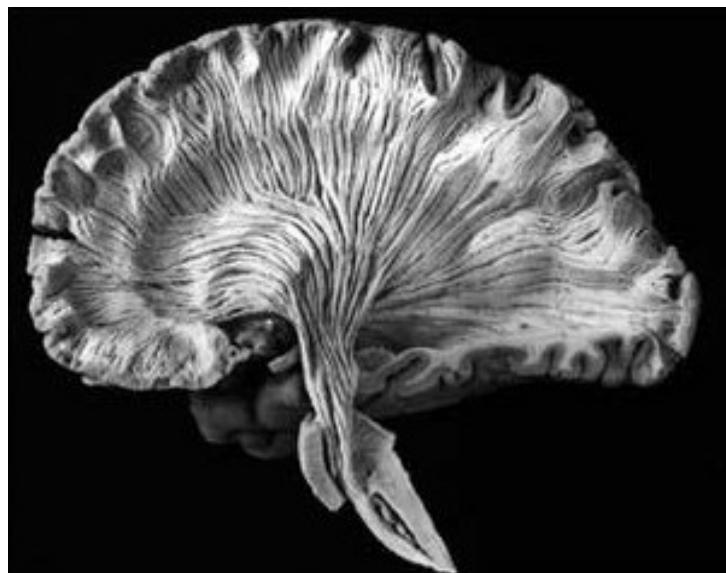
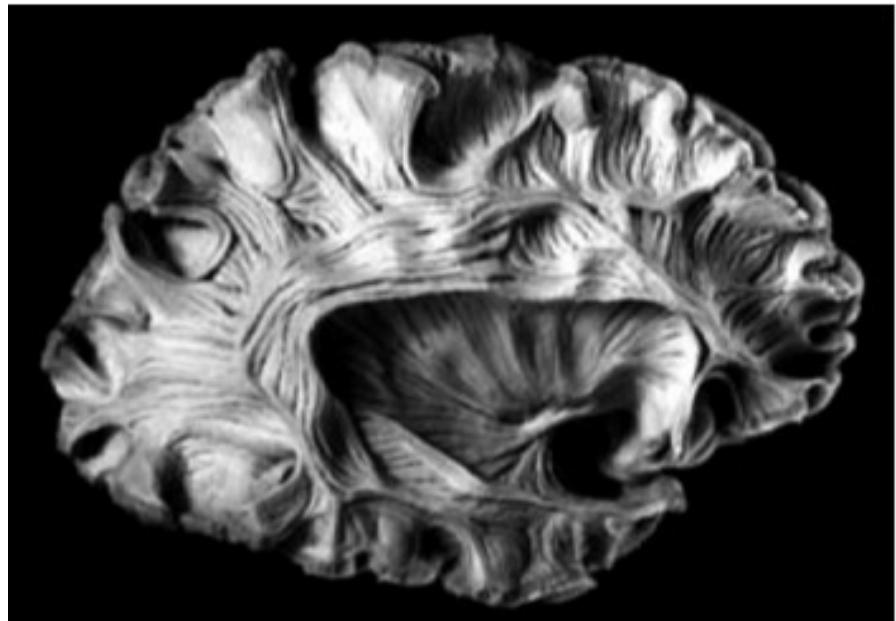
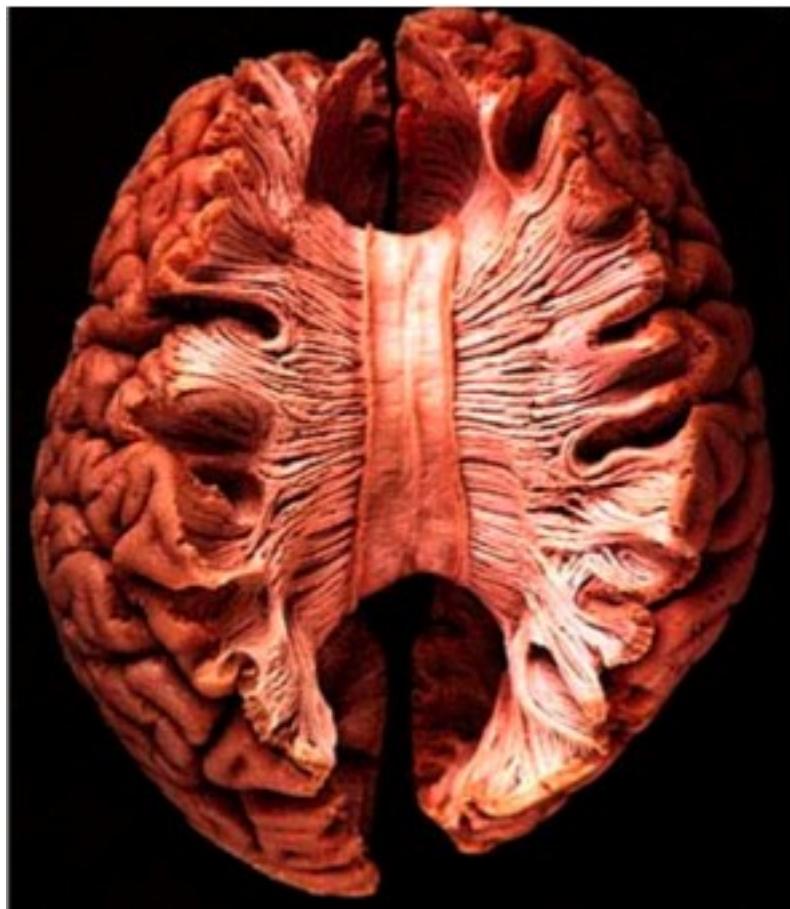
PhD Defense
21 Oct 2010



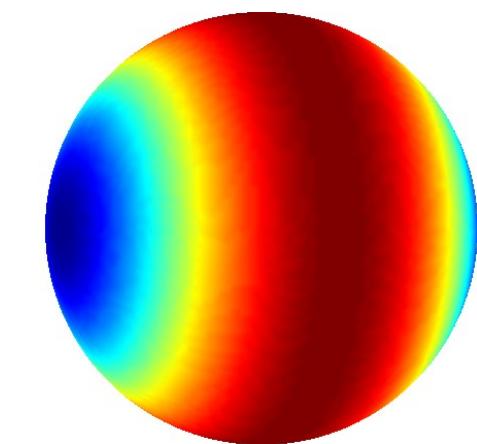
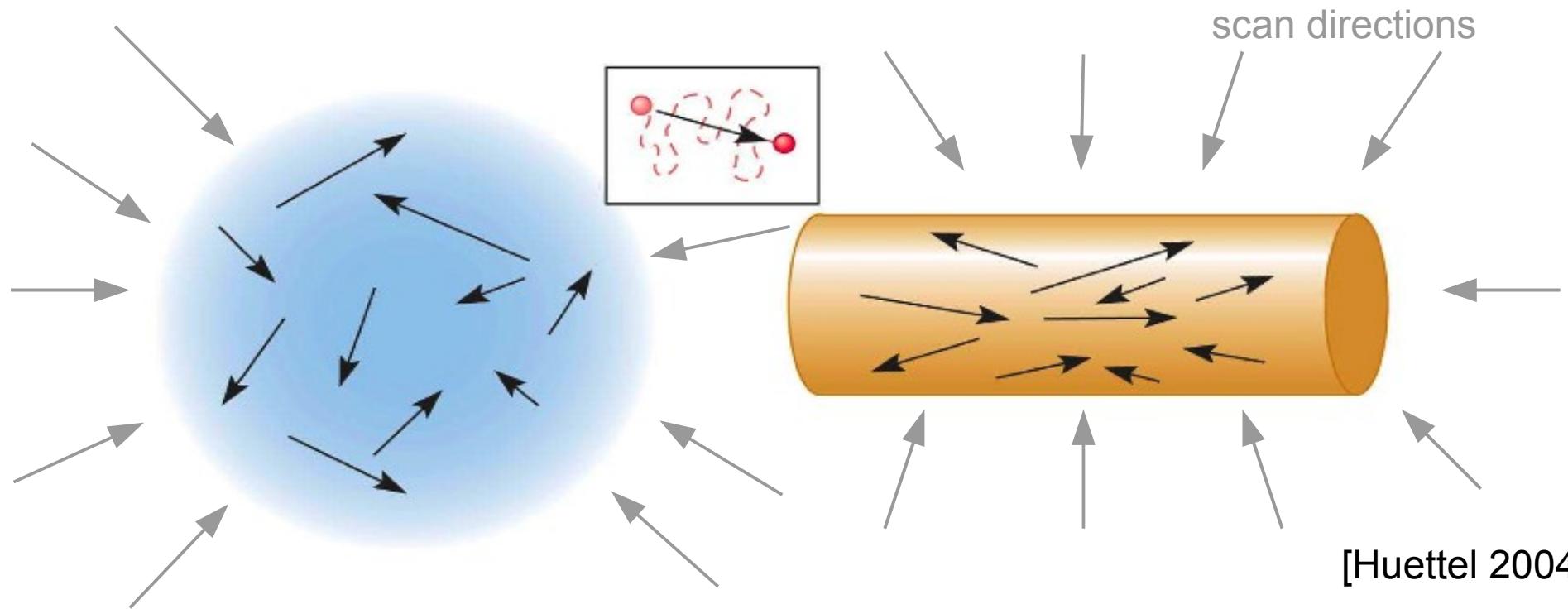
background

J. G. Malcolm, Y. Rathi, and C.-F. Westin. “Processing and visualization of diffusion MRI.” In T. Deserno, editor, *Recent Advances in Biomedical Image Processing and Analysis*, chapter 16, pages 387–410. Springer, 2011.

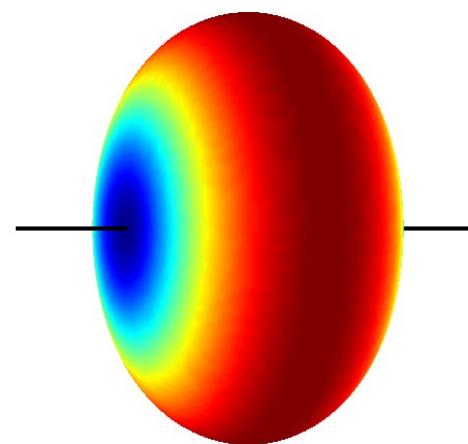
neural fibers



[Williams 97]⁴



isotropic scanner signal

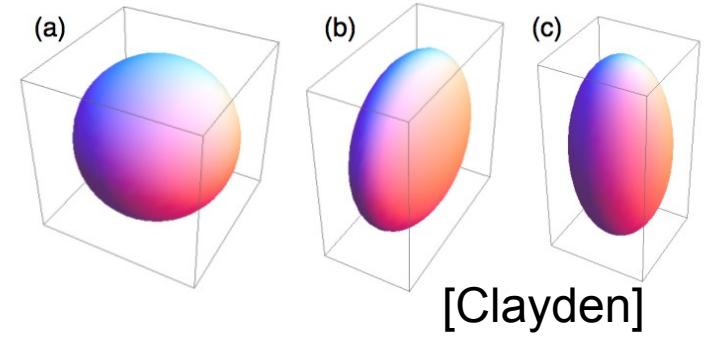


directed signal

imaging techniques

- Diffusion tensor imaging (DTI)
single-tensor

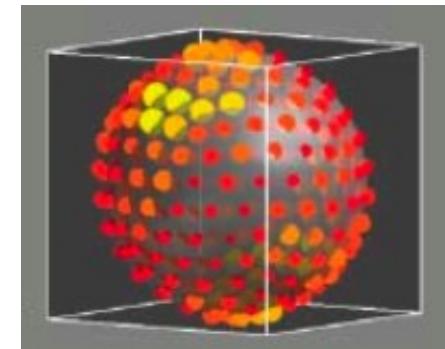
[Basser 94]



[Clayden]

- High Angular Resolution (QBI)
multi-fiber

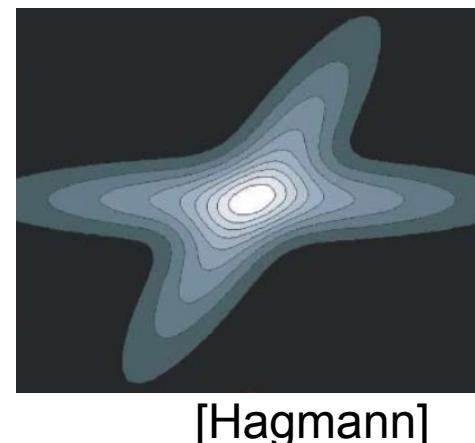
[Tuch 02]



[Tuch]

- Diffusion Spectrum (DSI)
radial information

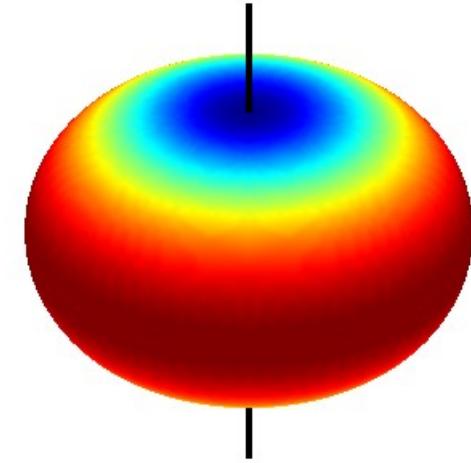
[Wedgeen 05, Hagmann 05]



[Hagmann]



one neural fiber
0.2 to 20 microns

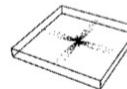
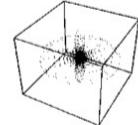
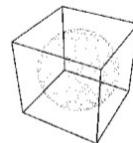


one scanned voxel
 $1.7 \times 1.7 \times 1.7$ mm

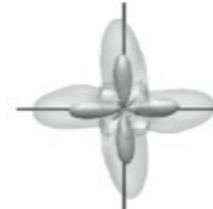
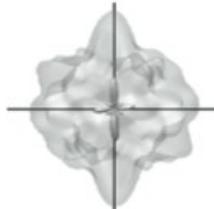
voxel reconstruction



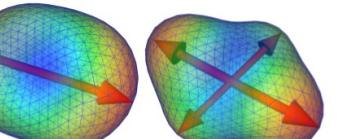
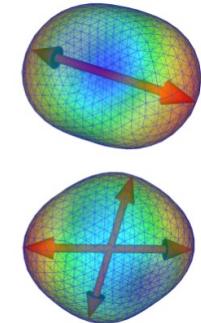
tensor mixtures [Tuch 02]



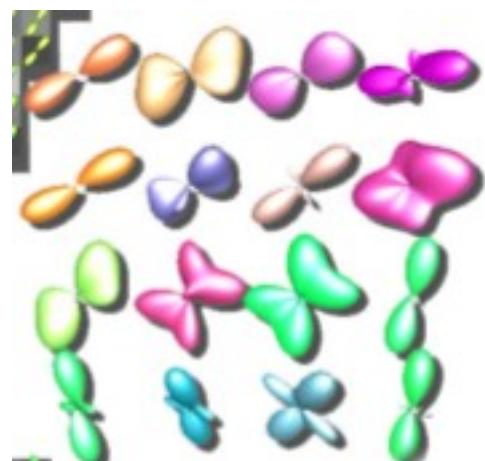
PAS [Jansons 03], MESD [Alexander 05]



SD [Tournier 04]



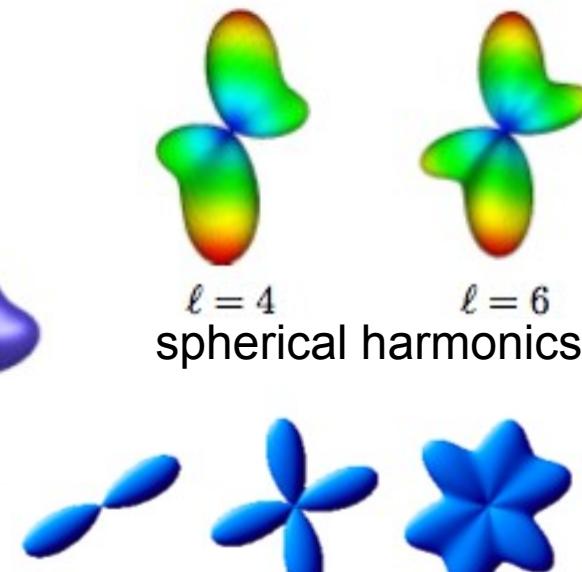
HOT [Hlawitschka 05]



VMF [Kumar 08]



DOT [Ozarslan 05]



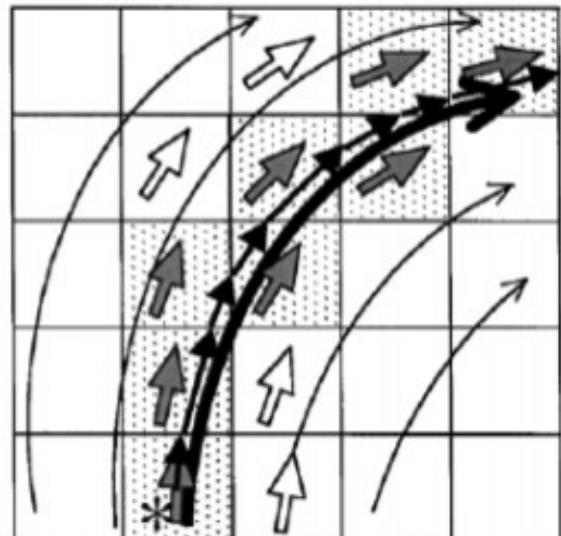
$\ell = 4$ $\ell = 6$ $\ell = 8$
spherical harmonics [Descoteaux 07]



Wishart [Jian 07]

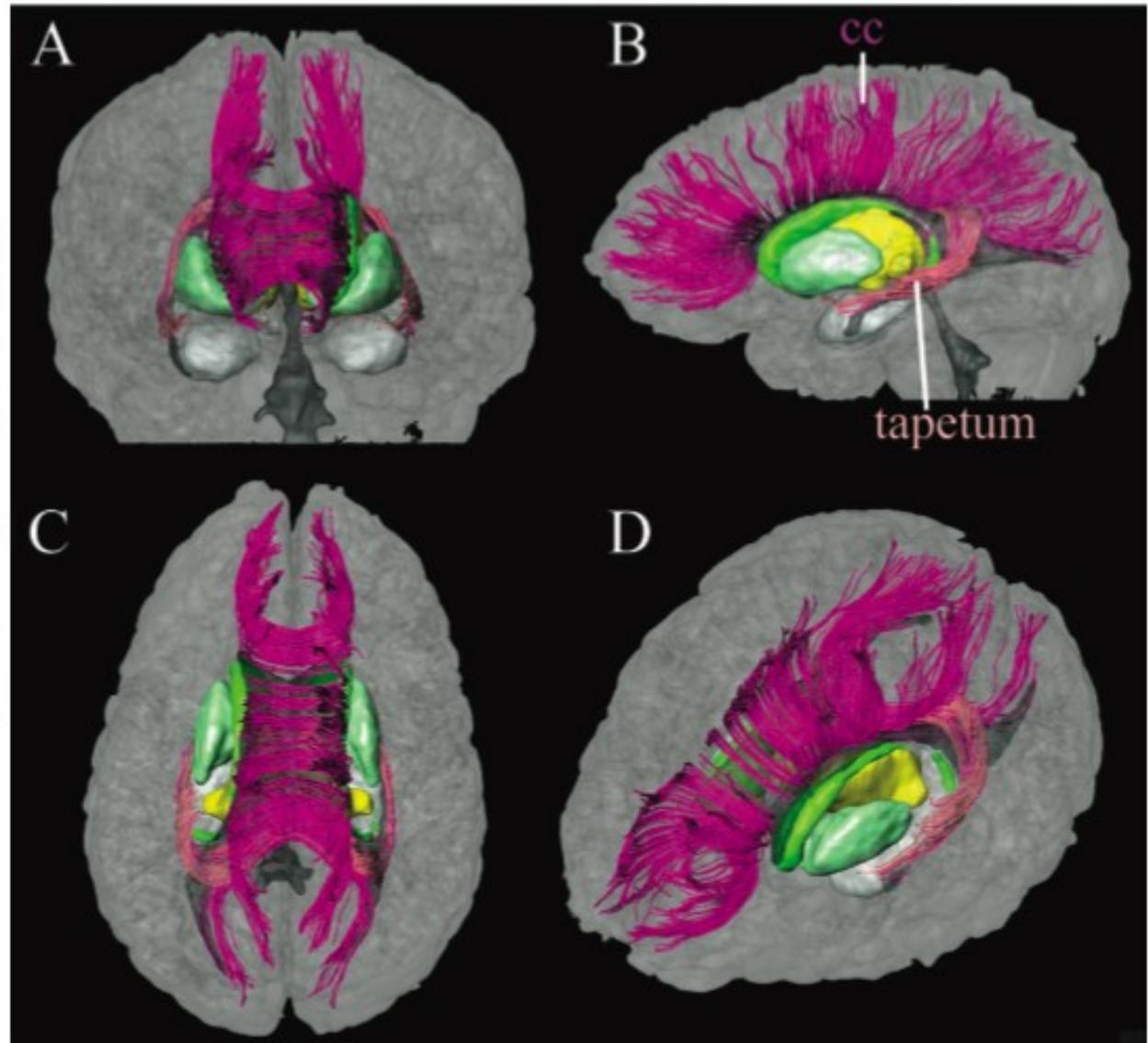
deterministic tractography

streamlin
e



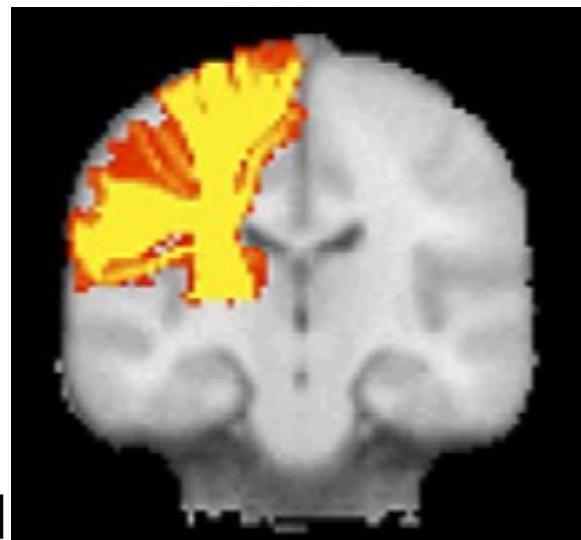
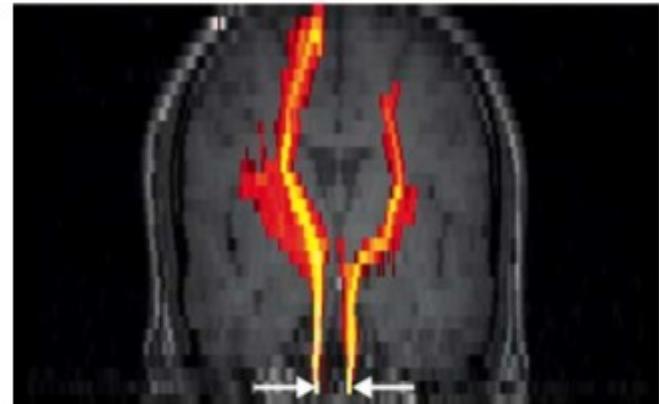
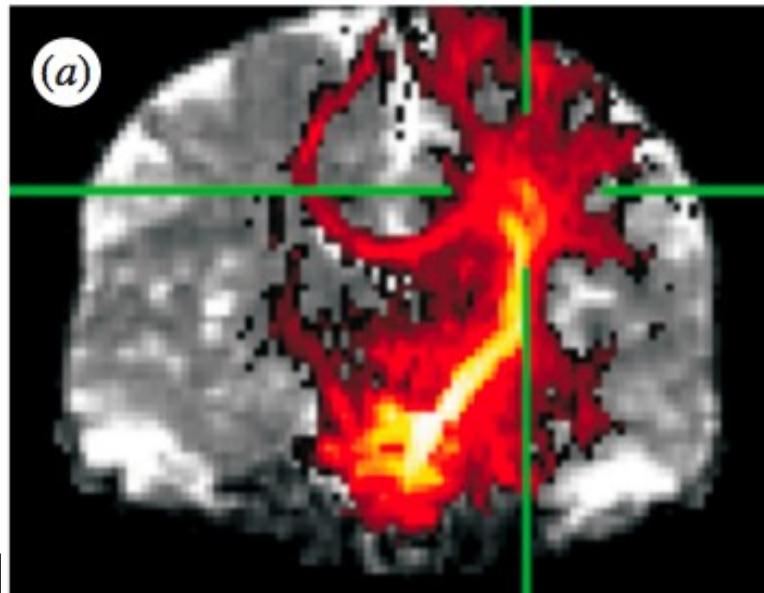
[Mori 99]

[Conturo 99, Basser 00]



[Wakana 03]

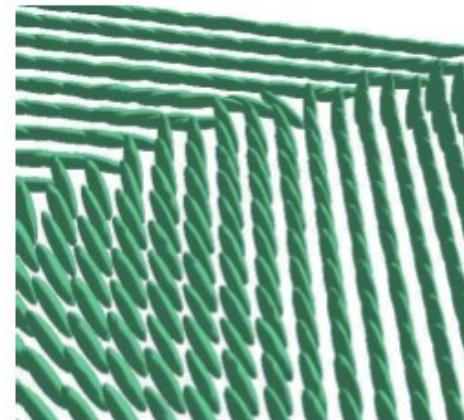
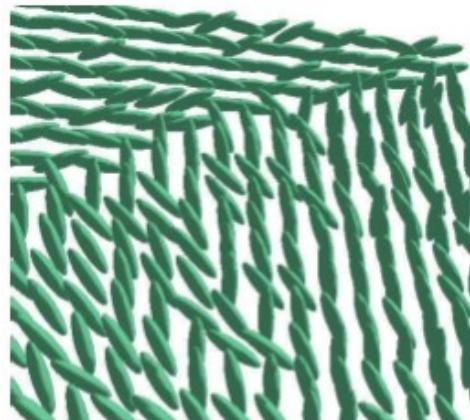
probabilistic tractography



[Friman 06]

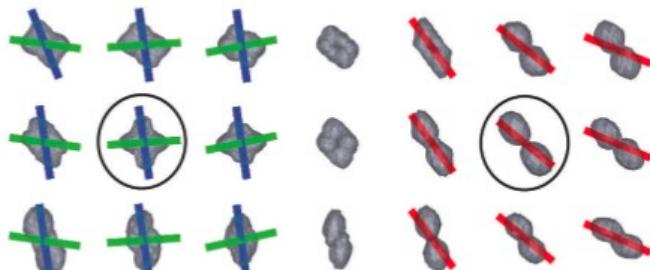
[Behrens 07]

spatial regularization

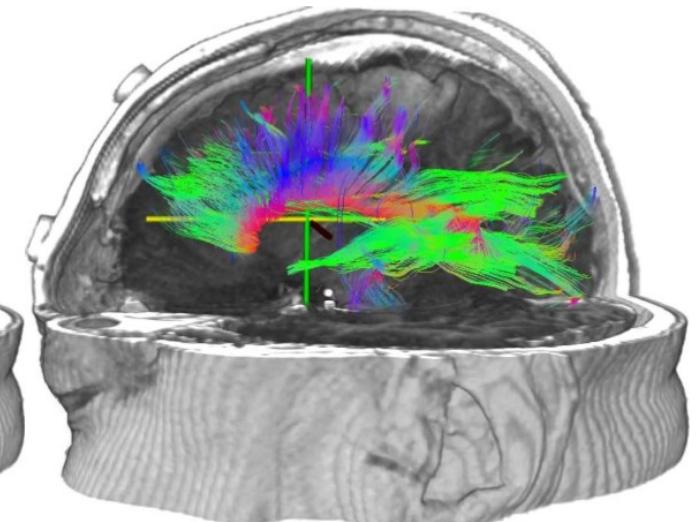
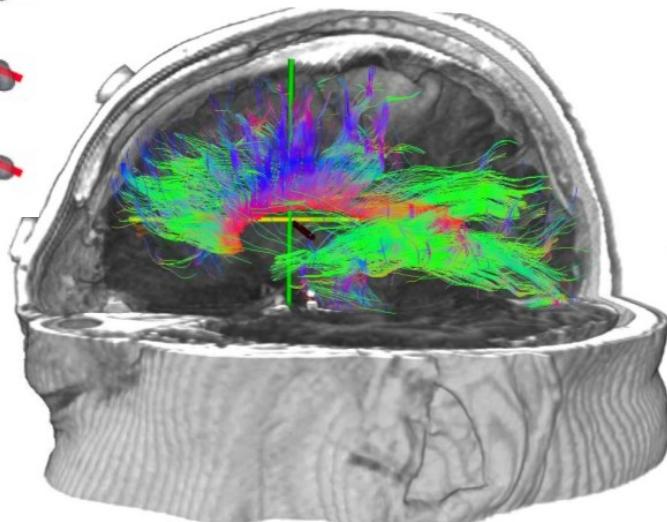


pre/post-processing

[Tschumperle 03]



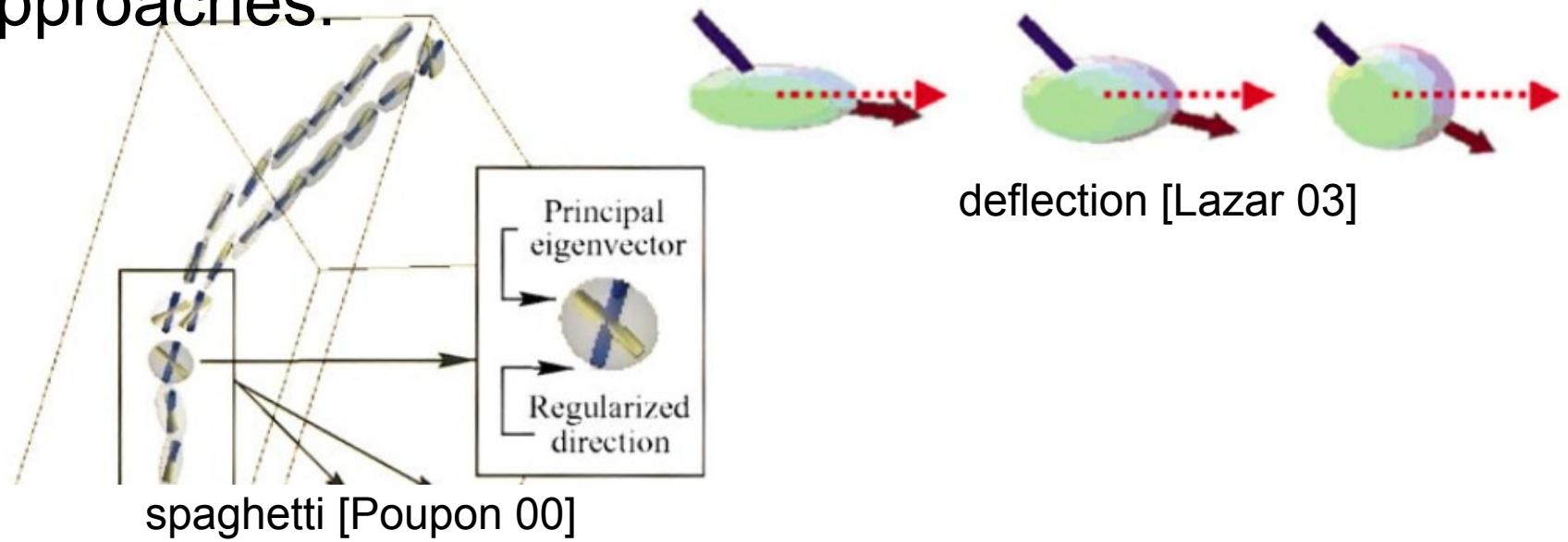
[Savadjiev 07]



[Fillard 07]

tract regularization

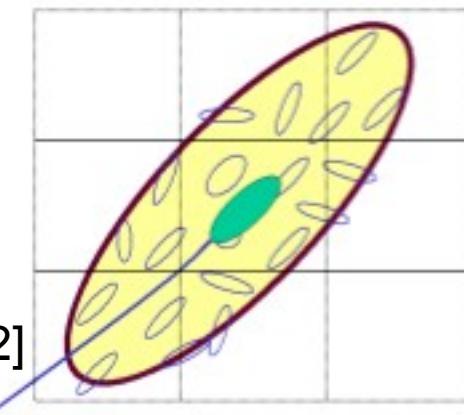
deterministic
approaches:



spaghetti [Poupon 00]

deflection [Lazar 03]

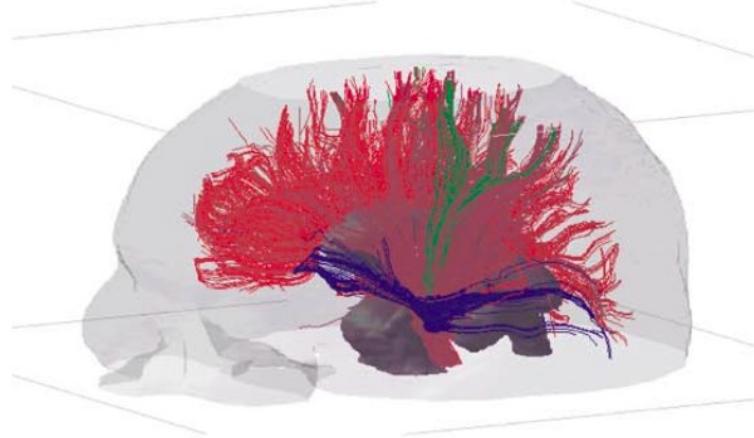
[Zhukov 02]



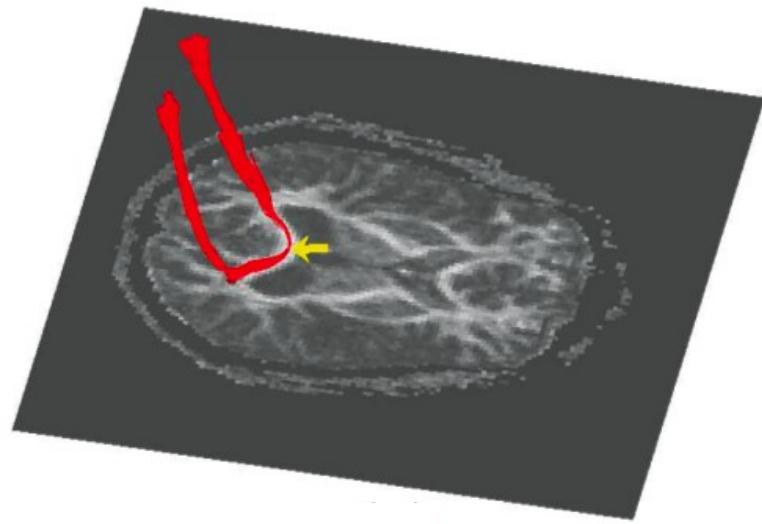
single-tensor
path
regularization

tract regularization

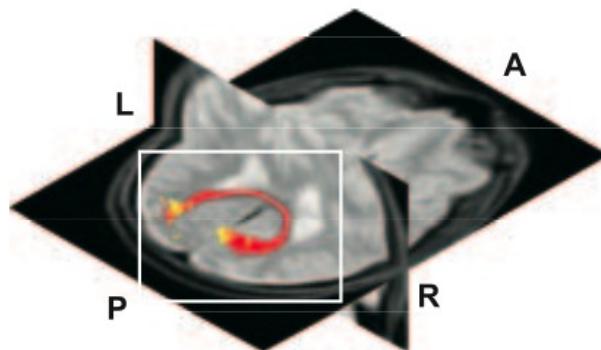
probabilistic
approaches:



linear Kalman filter [Gossl 02]



particle filtering [Zhang 07]



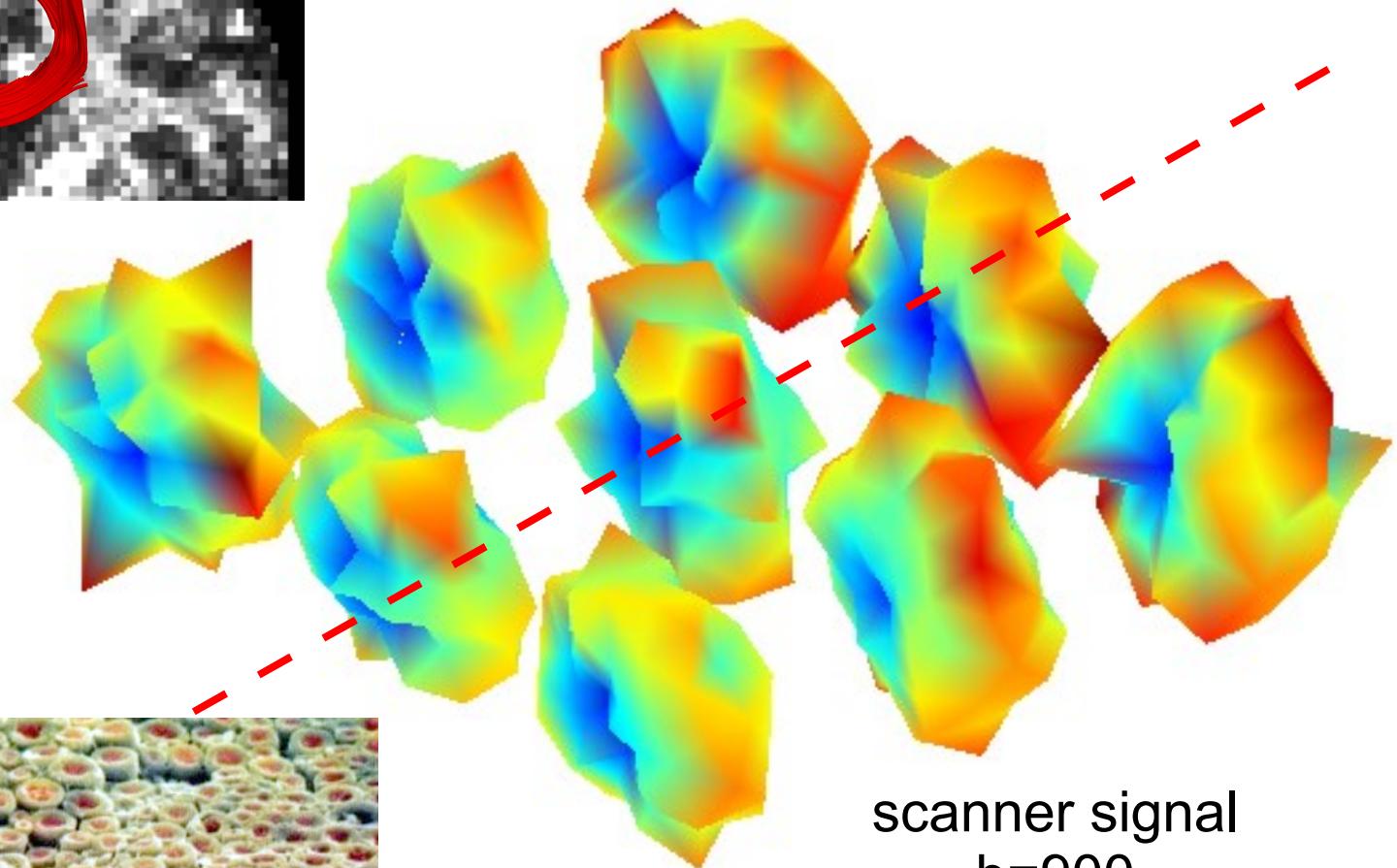
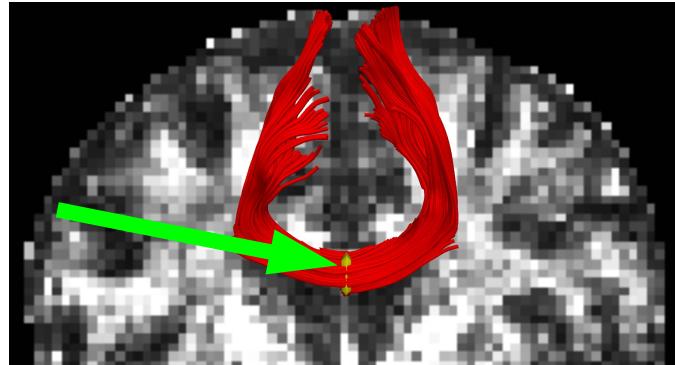
stochastic [Bjornemo 02]

single-tensor
path
regularization

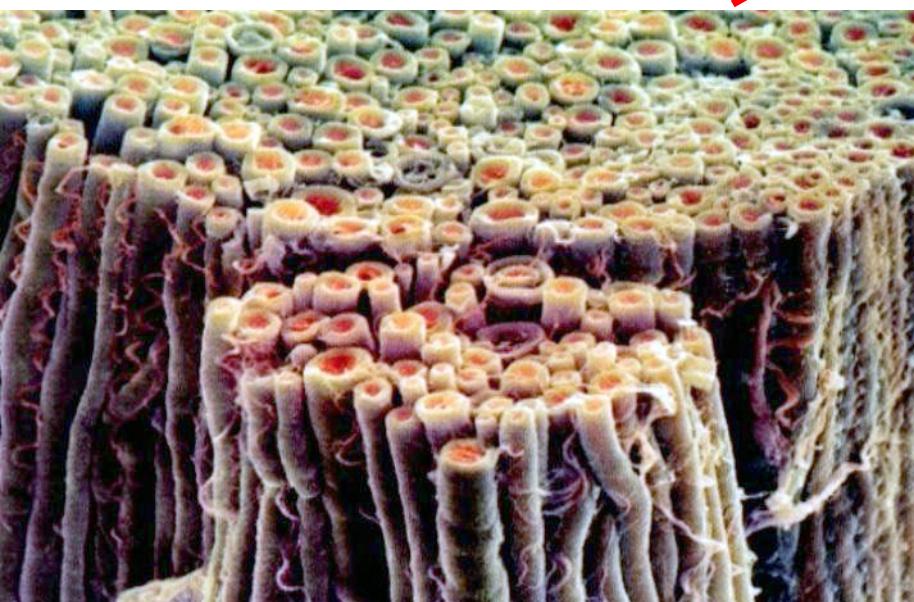
method: the model

Y. Rathi, J. G. Malcolm, O. Michailovich, C.-F. Westin, M. E. Shenton, and S. Bouix. Tensor-kernels for simultaneous fiber model estimation and tractography. *Magnetic Resonance in Medicine*, 64(1):138–148, 2010.

J. G. Malcolm, M. E. Shenton, and Y. Rathi. Neural tractography using an unscented Kalman filter. In *Information Processing in Medical Imaging (IPMI)*, pages 126–138, 2009.



scanner signal
 $b=900$
51 directions
1.7mm isotropic voxel
17 minute scan



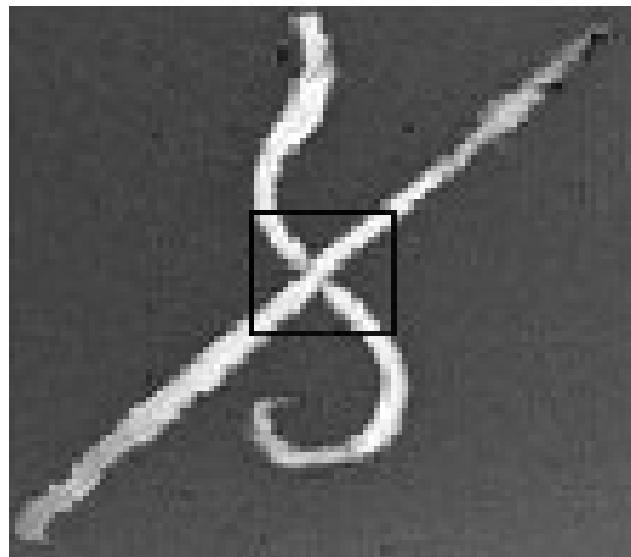
[Bartzokis]

DTI

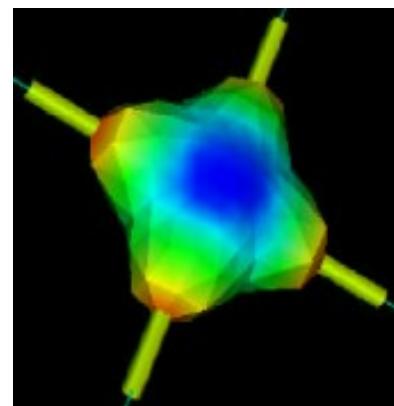
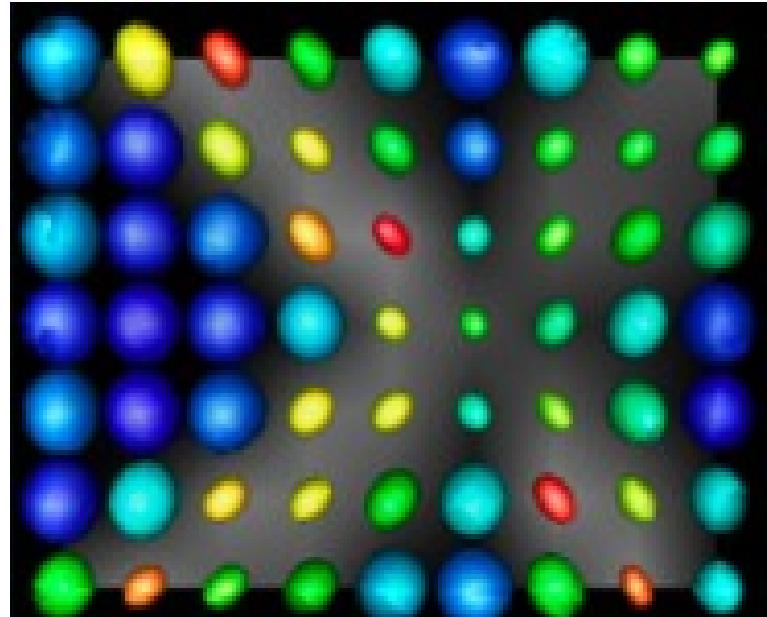
$$S(\mathbf{u}) = S_0 e^{-b \mathbf{u}^T D \mathbf{u}}$$

D	diffusion tensor	6 parameters
\mathbf{u}	unit direction	
b	acquisition constant	
S_0	null signal ($b=0$)	

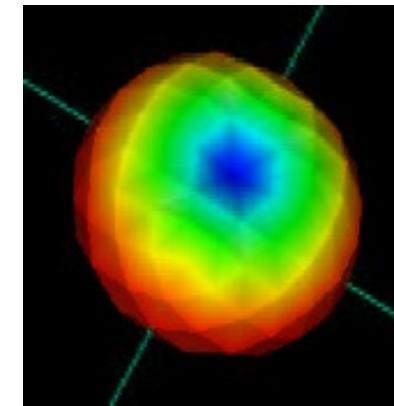
single-tensor limitations



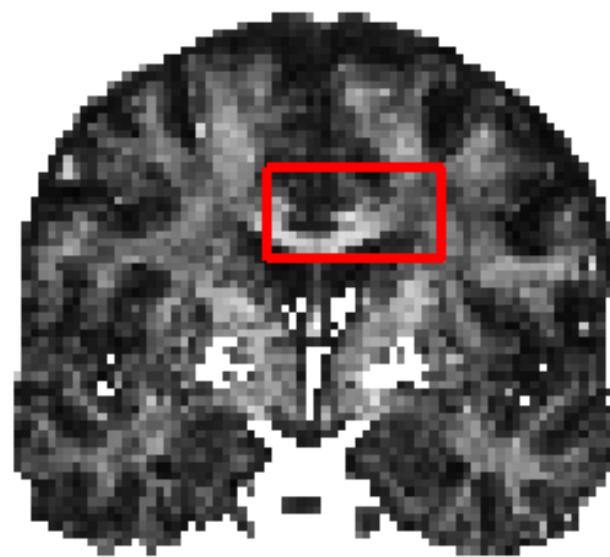
rat spinal nerves

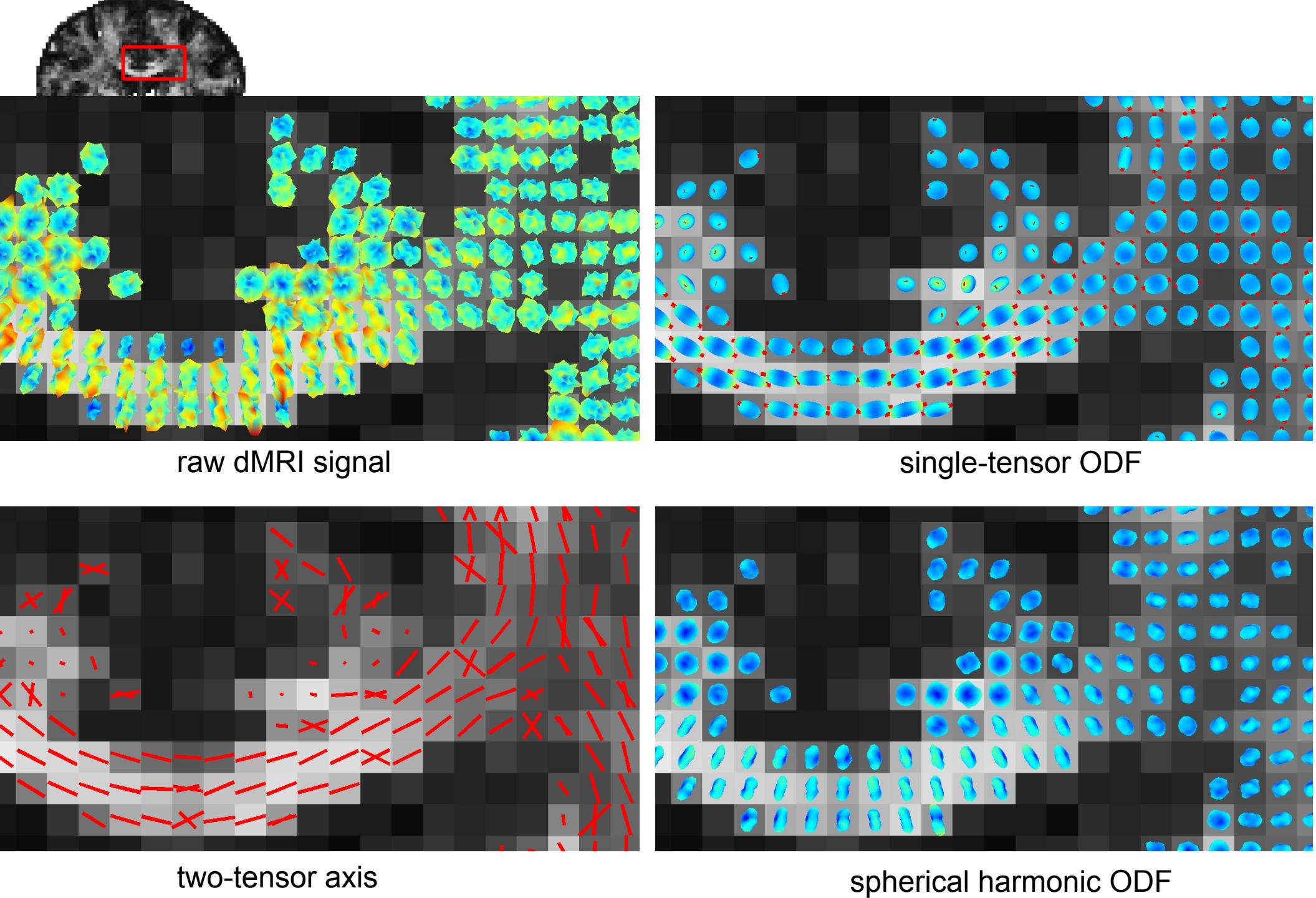


true ODF



single-tensor ODF





multi-tensor signal model

$$S(\mathbf{u}) = s_0 \sum_j w_j e^{-b \mathbf{u}^T D_j \mathbf{u}}$$

D_j diffusion tensor

\mathbf{u} unit direction

w_j convex weights

b acquisition constant

s_0 null signal ($b=0$)

model assumptions

...for now

Two fibers

Fixed volume fractions

Tensors are elliptic or isotropic

model parameters

for two fibers...

...two principal directions $m \in \mathbb{R}^3$

...two primary eigenvalues $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues $\lambda_2 \in \mathbb{R}$

5 + 5 = 10 parameters

model parameters

for two fibers...

...two principal directions $\mathbf{m} \in \mathbb{R}^3$

...two primary eigenvalues $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues $\lambda_2 \in \mathbb{R}$

5 + 5 = 10 parameters

$$S(\mathbf{u}) = 0.5 s_0 e^{-b \mathbf{u}^T D_1 \mathbf{u}} + 0.5 s_0 e^{-b \mathbf{u}^T D_2 \mathbf{u}}$$

$$D_1 = \lambda_{11} \mathbf{m}_1 \mathbf{m}_1^T + \lambda_{21} (\mathbf{p} \mathbf{p}^T + \mathbf{q} \mathbf{q}^T)$$

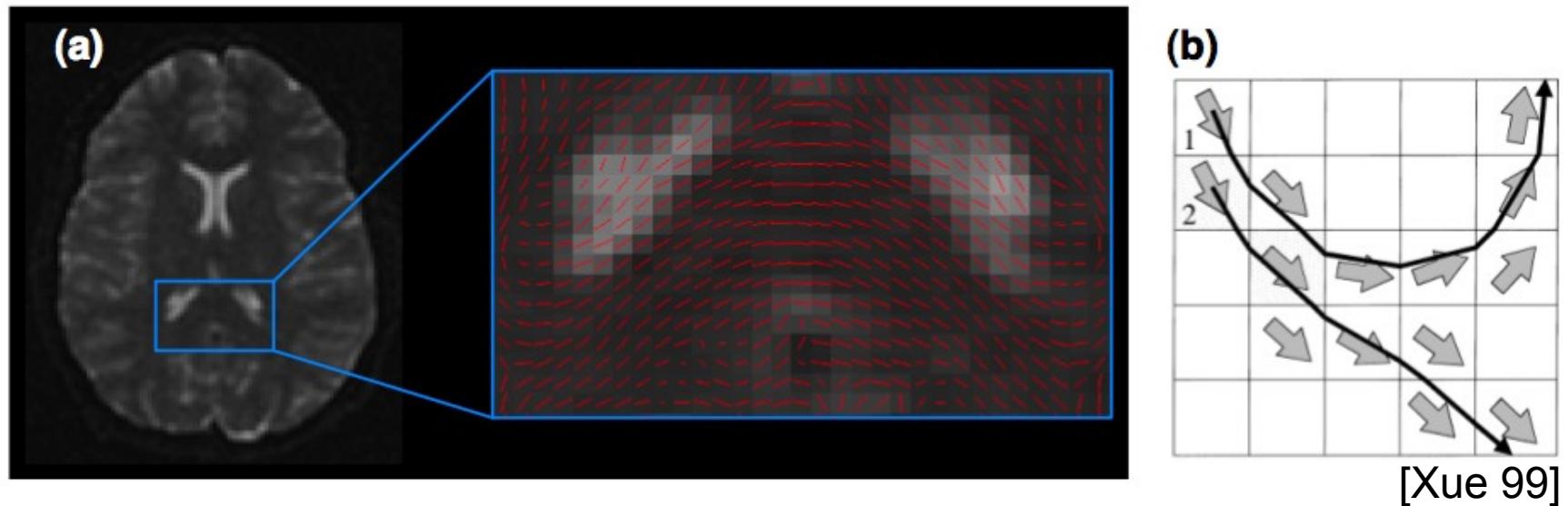
eigenvectors: $\mathbf{m}, \mathbf{p}, \mathbf{q}$

method: estimating the model

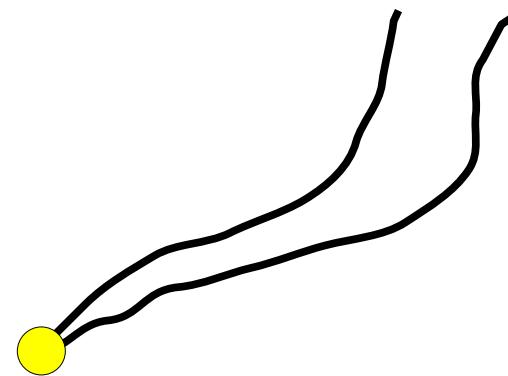
J. G. Malcolm, O. Michailovich, S. Bouix, C.-F. Westin, M. E. Shenton, and Y. Rathi. A filtered approach to neural tractography using the Watson directional function. *Medical Image Analysis*, 14:58–69, 2010.

J. G. Malcolm, M. E. Shenton, and Y. Rathi. Filtered multi-tensor tractography. *IEEE Trans. on Medical Imaging*, 29:1664–1675, 2010.

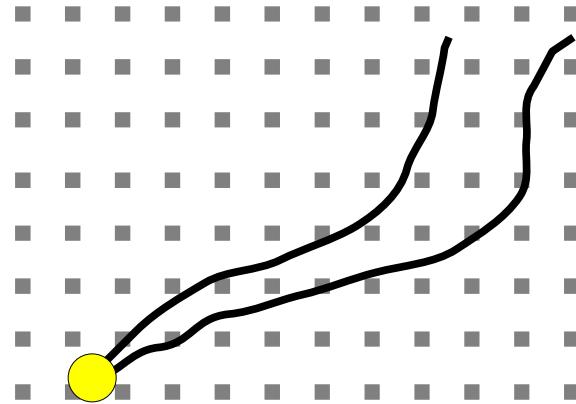
independent estimation



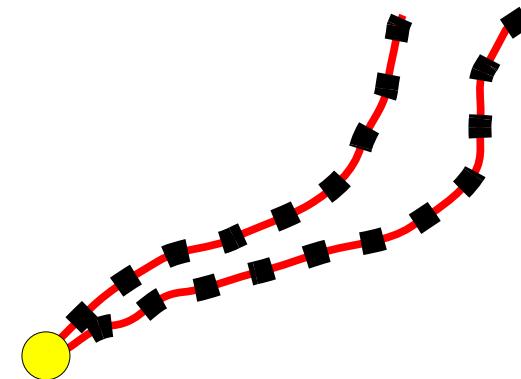
the system: a fiber



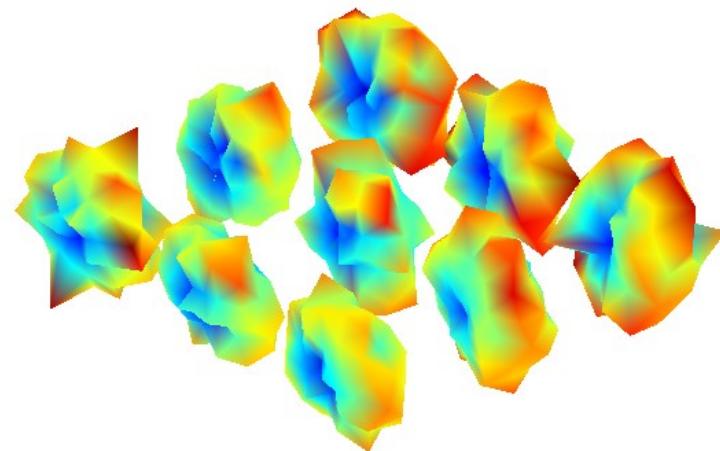
**independent
process**



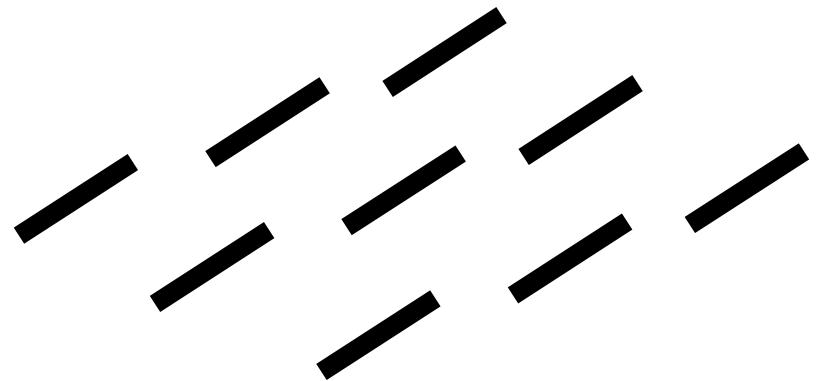
**causal
process**



model-based filtering



scanner
measurement



underlying
model

objectives:

- estimate model from measurements
- suppress noise

notation

\boldsymbol{x}_t state of system at time t
state = “model parameters”

\boldsymbol{y}_t what you see at time t
observation, measurement

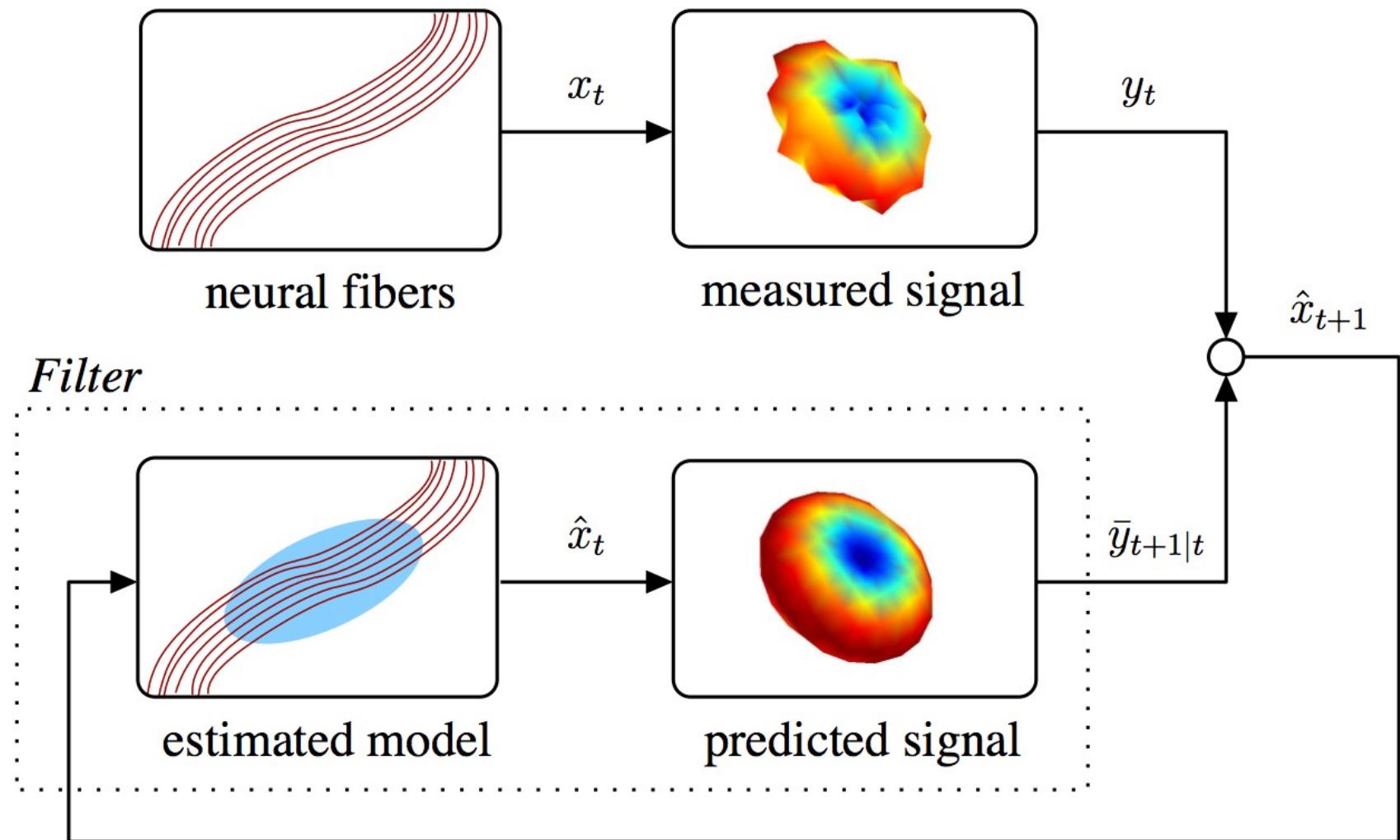
update: $\boldsymbol{x}_{t+1} = F \boldsymbol{x}_t$ $\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t)$

observation: $\boldsymbol{y}_t = G \boldsymbol{x}_t$ $\boldsymbol{y}_t = g(\boldsymbol{x}_t)$

linear

nonlinear

Kalman filtering



predict ... measure ... reconcile ... repeat ...

$$\begin{aligned} \boldsymbol{x} &= [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10} \\ y &\in R^m \text{ signal} \quad \begin{matrix} 10 \text{ dimensional} \\ \text{state} \end{matrix} \end{aligned}$$

$$\boldsymbol{x} = [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

10 dimensional
state

$$y \in R^m \text{ signal}$$

$$\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t) = \boldsymbol{x}_t$$

small steps
slowly varying
state

$$y_t = g(\boldsymbol{x}_t) = S(\boldsymbol{u})$$

$$\boldsymbol{x} = [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

$$y \in R^m \text{ signal}$$

10 dimensional
state

$$\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t) = \boldsymbol{x}_t$$

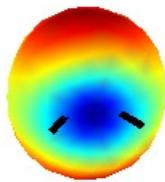
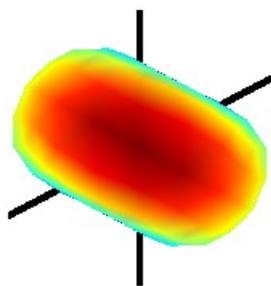
small steps
slowly varying
state

$$y_t = g(\boldsymbol{x}_t) = S(\boldsymbol{u})$$

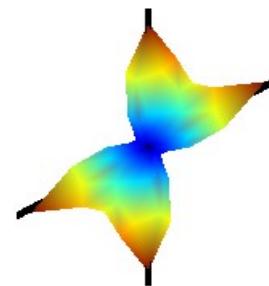
$$y(\boldsymbol{u}) = S(\boldsymbol{u}) = 0.5 s_0 e^{-b\boldsymbol{u}^T D_1 \boldsymbol{u}} + 0.5 s_0 e^{-b\boldsymbol{u}^T D_2 \boldsymbol{u}}$$

$$D = \lambda_1 \boldsymbol{m} \boldsymbol{m}^T + \lambda_2 (\boldsymbol{p} \boldsymbol{p}^T + \boldsymbol{q} \boldsymbol{q}^T)$$

Local fiber model: mixture of two tensors



diffusion MRI signal



orientation distribution
function (ODF)

signal reconstruction is nonlinear

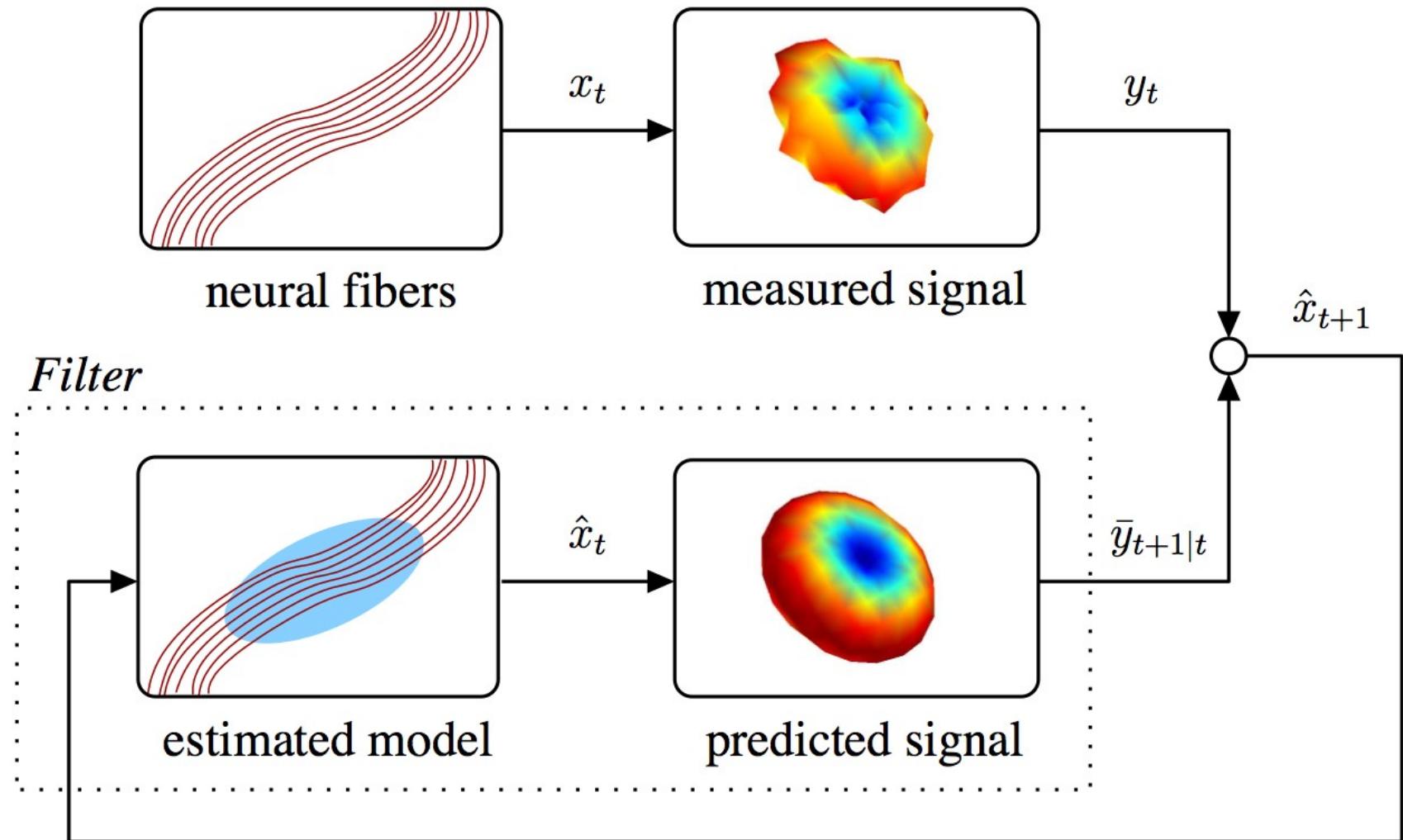
independent optimization

- least squares
linearization
- gradient descent
local minima
- Levenberg-Marquardt
local minima

causal estimation

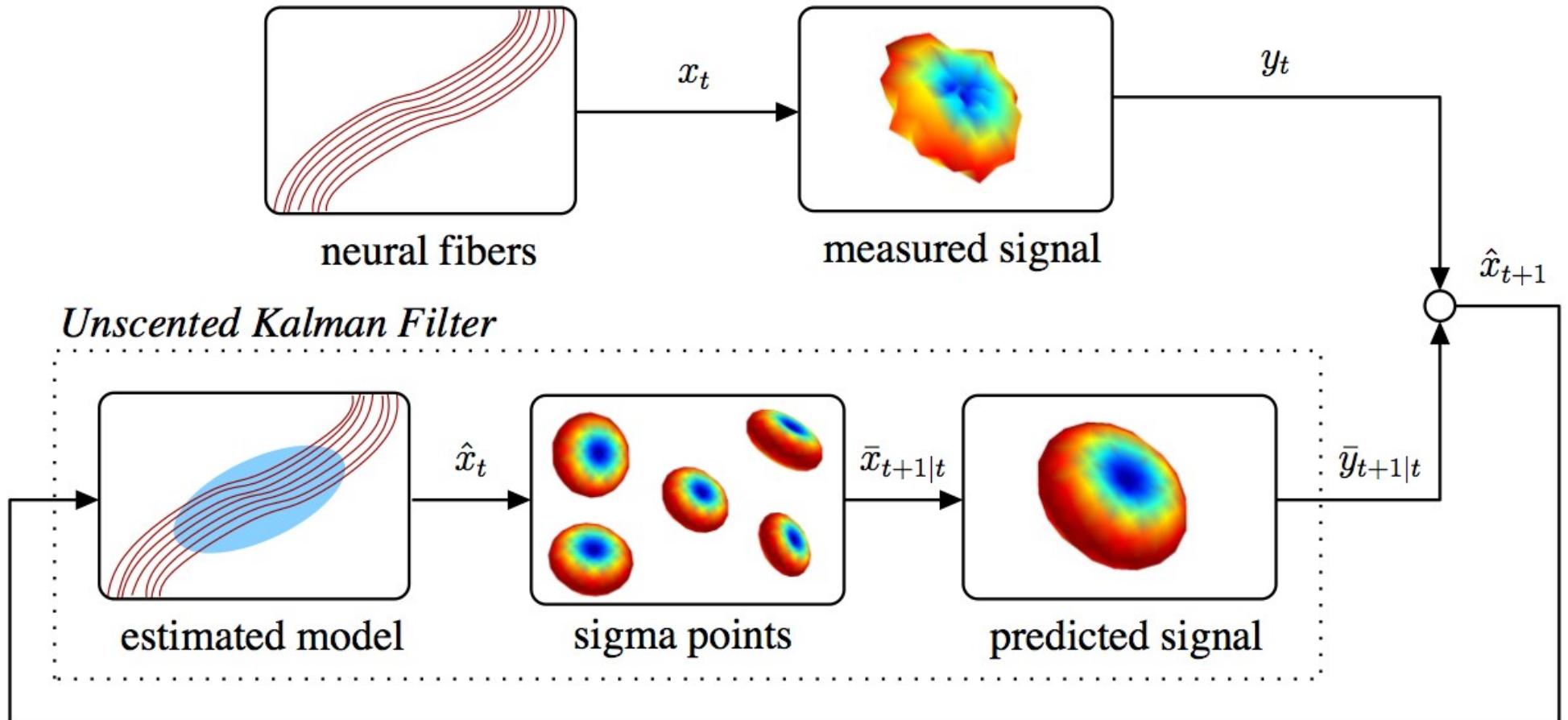
- extended Kalman filter
mean + covariance
linearization
- particle filter
non-parametric
sampling
- unscented Kalman filter
mean + covariance
no linearization
limited sampling

linear Kalman filter



predict ... measure ... reconcile ... repeat ...

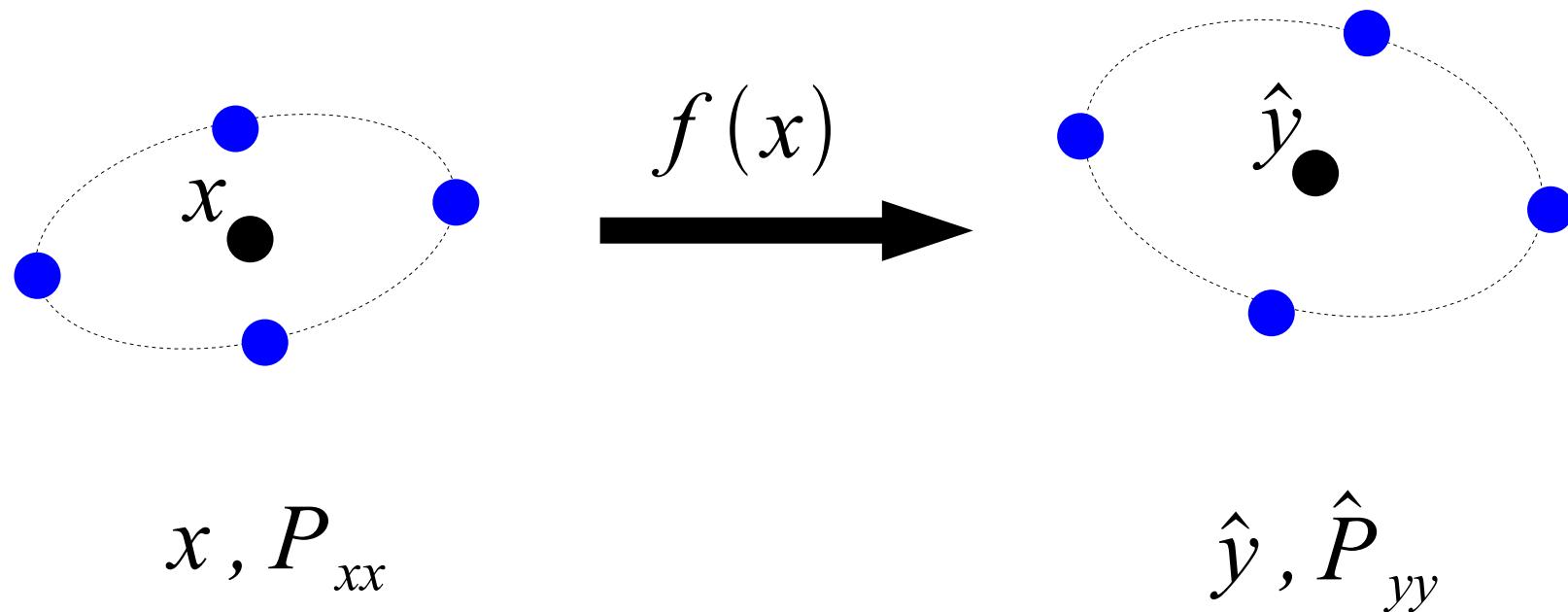
unscented Kalman filter



same update equations
modified prediction step

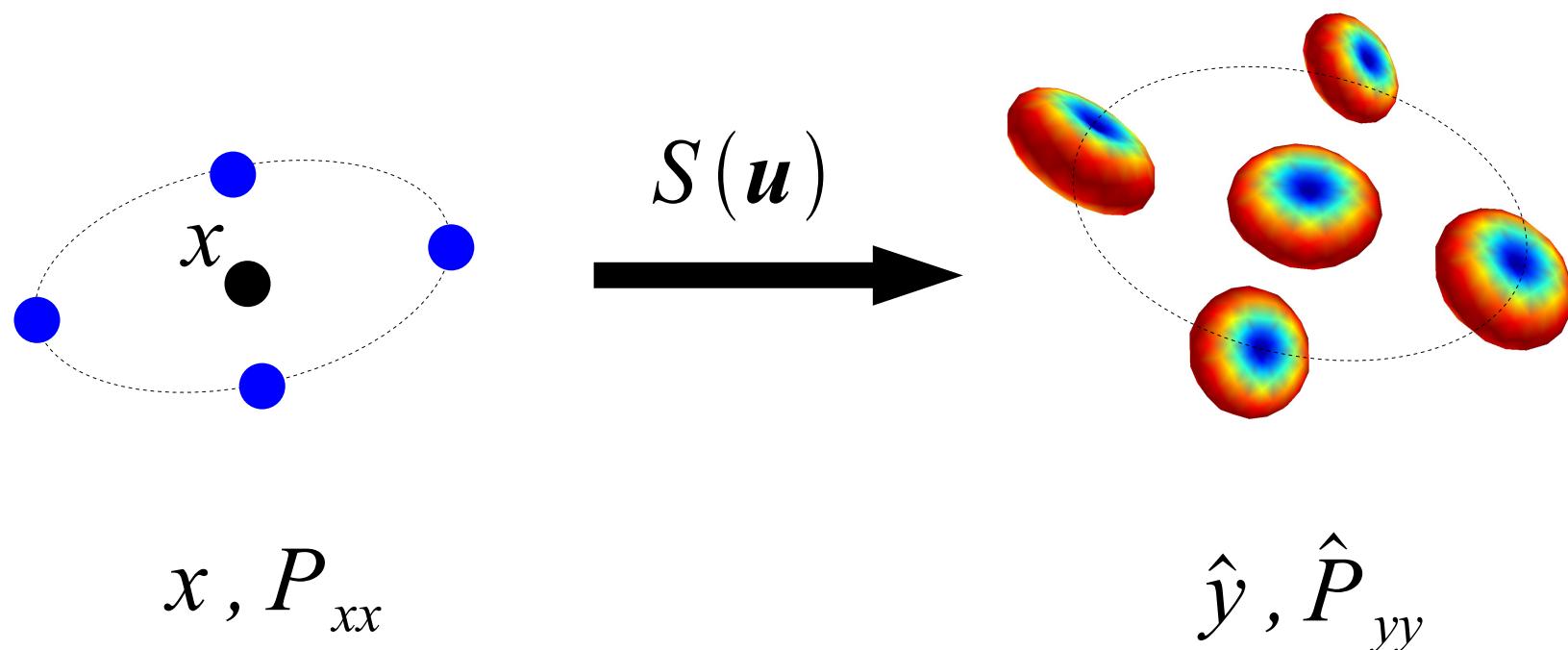
unscented transform

approximate the statistics...not the function



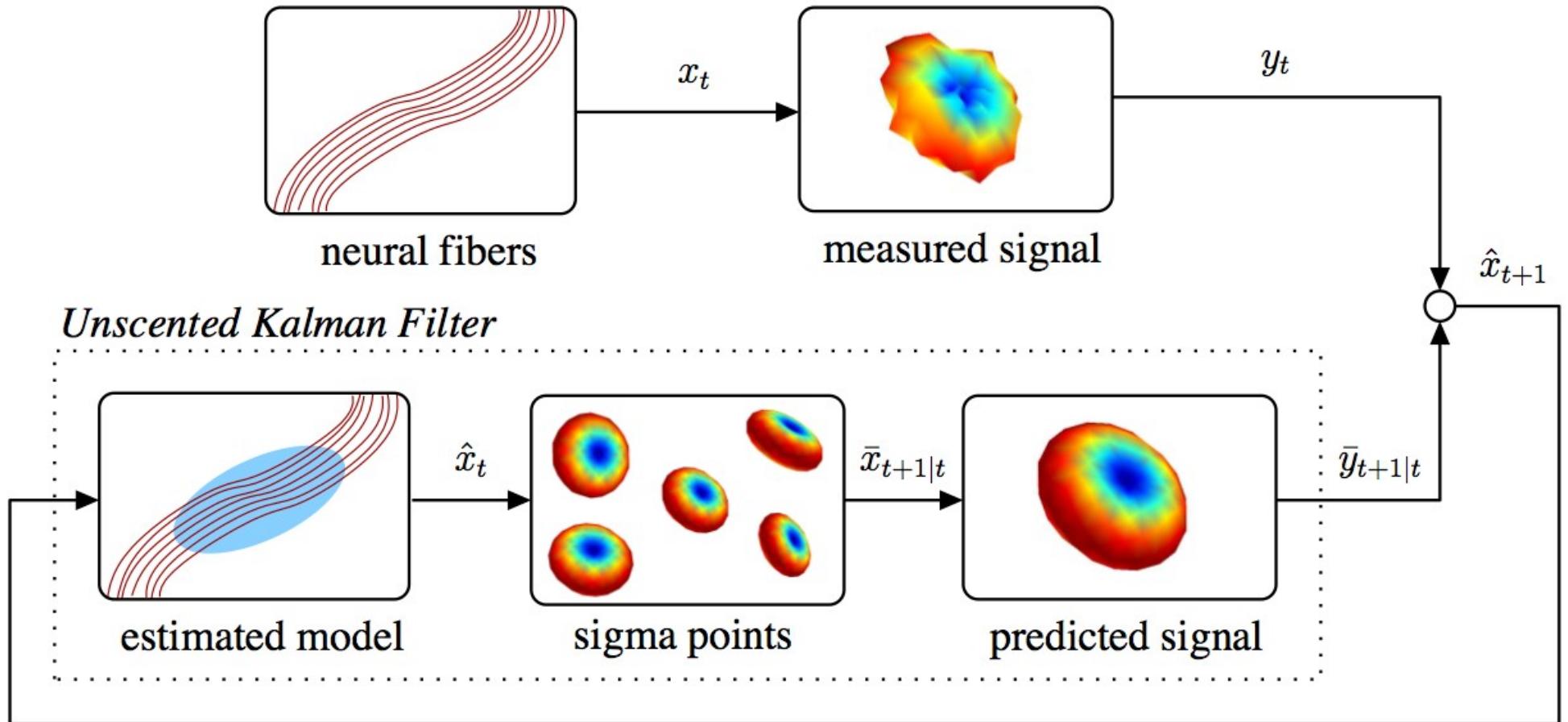
unscented transform

for signal reconstruction...



$$\boldsymbol{x} = [\boldsymbol{m}_1 k_1 \boldsymbol{m}_2 k_2]^T \in R^8$$

unscented Kalman filter

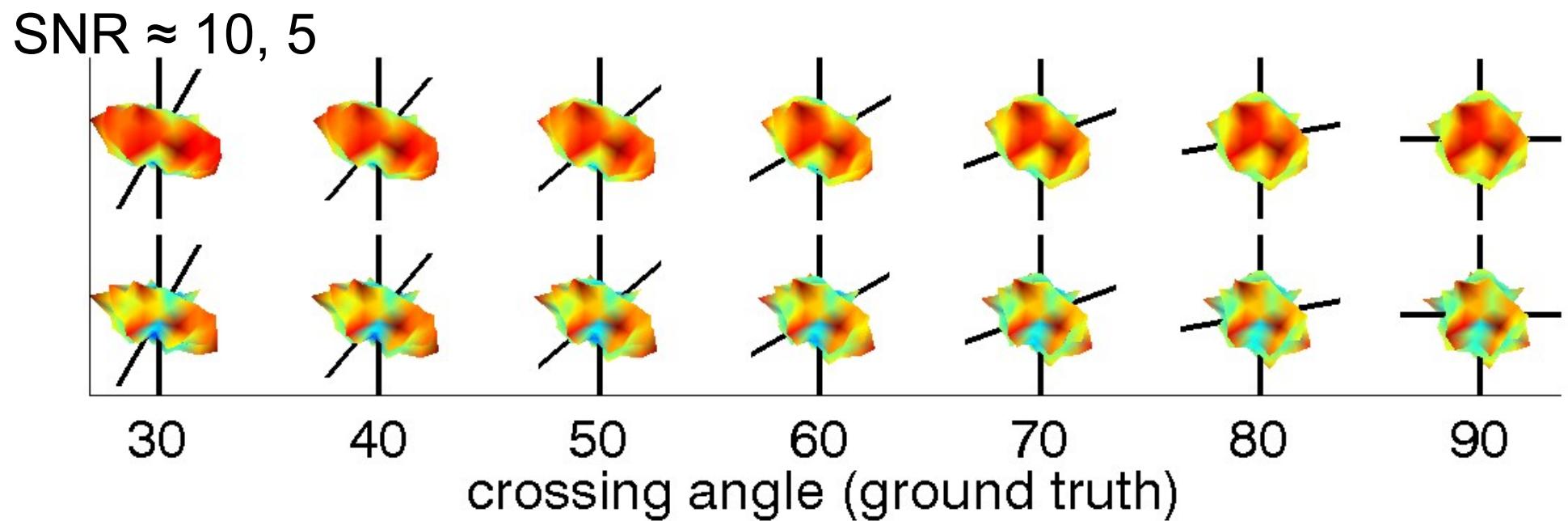
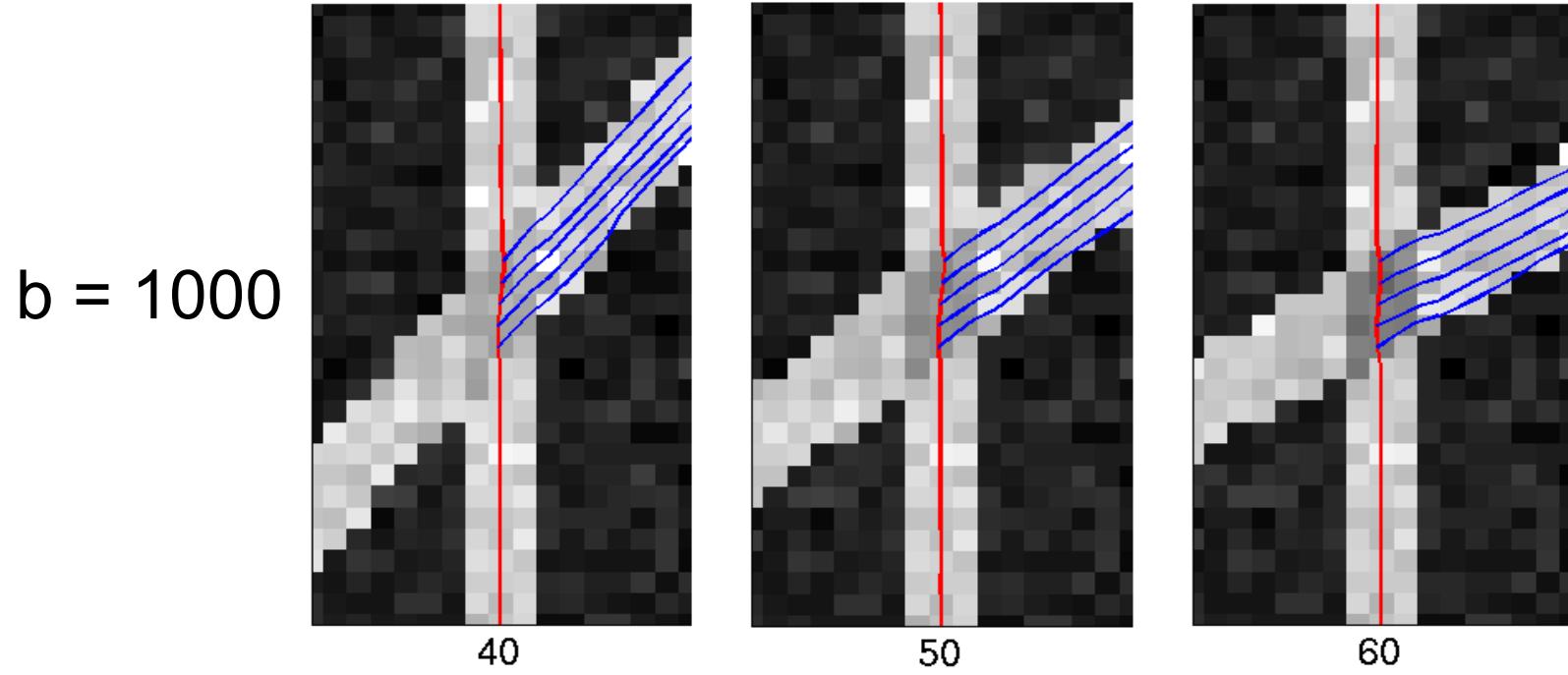


predict ... measure ... reconcile ... repeat ...

diffusion tensor results

J. G. Malcolm, M. E. Shenton, and Y. Rathi. Filtered multi-tensor tractography. *IEEE Trans. on Medical Imaging*, 29:1664–1675, 2010.

synthetic validation



nonlinear least squares

- Levenberg-Marquart
- two-tensor model
- initialize with ground truth (best possible)

spherical harmonics

- non-parametric
- order eight (8)
- fiber sharpening for peak detection ($L=0.006$)

filtered tractography

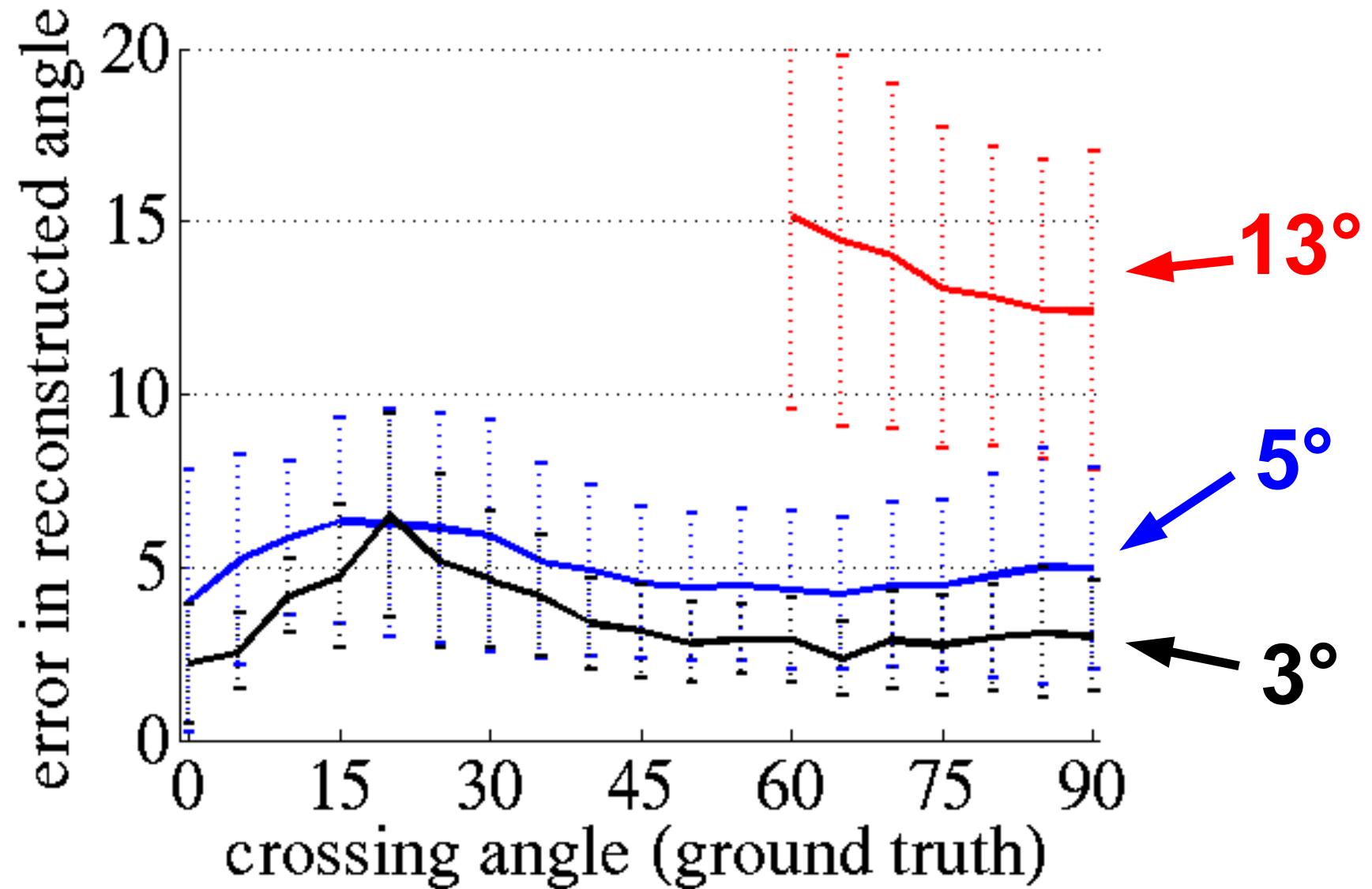
- two-fiber model
- unscented Kalman filter

[Descoteaux 07]

J. G. Malcolm, M. E. Shenton, and Y. Rathi. Neural tractography using an unscented Kalman filter. In *Information Processing in Medical Imaging (IPMI)*, pages 126–138, 2009.

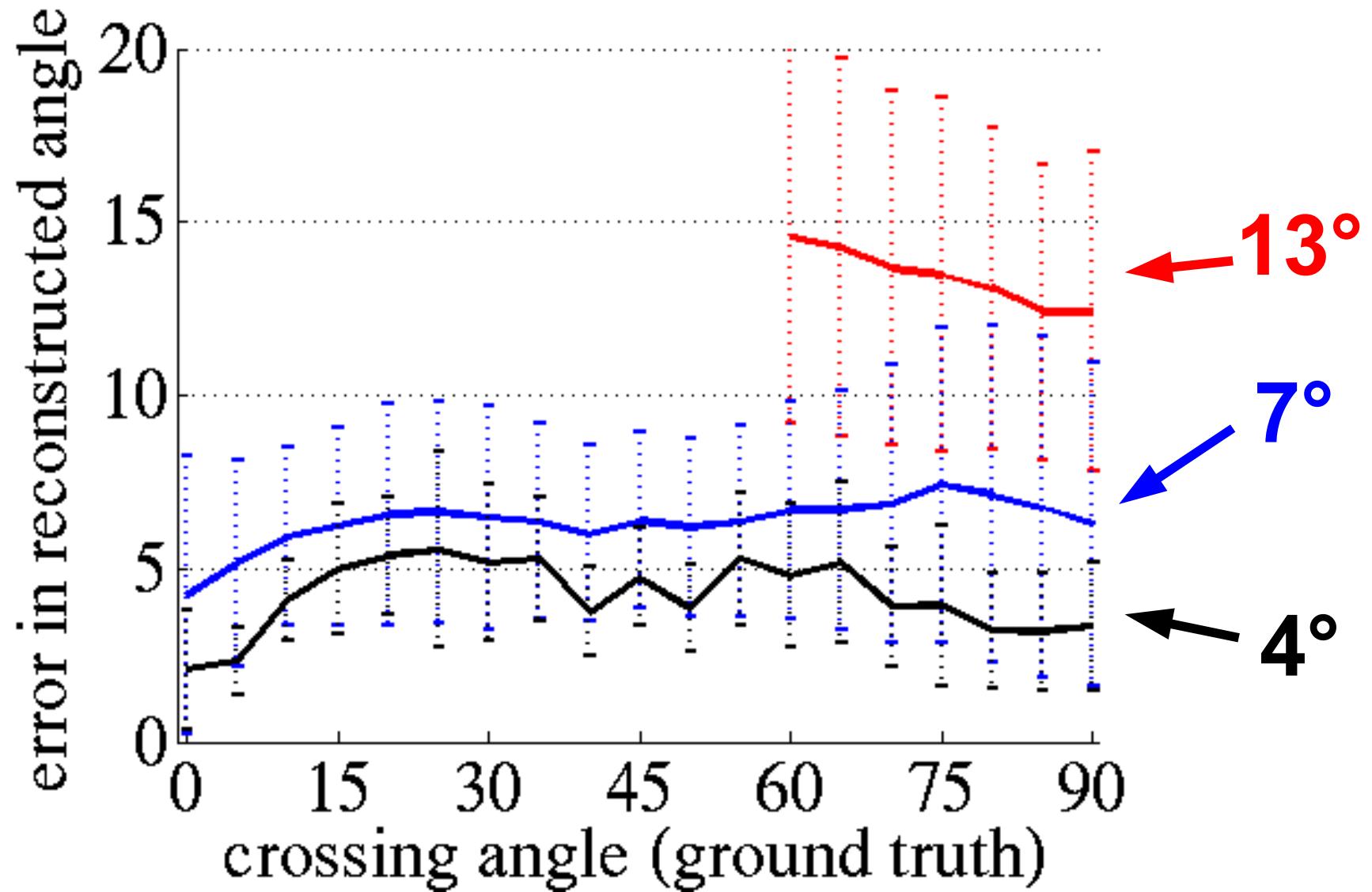
J. G. Malcolm, M. E. Shenton, and Y. Rathi. Filtered multi-tensor tractography. *IEEE Trans. on Medical Imaging*, 29:1664–1675, 2010.

angular reconstruction error



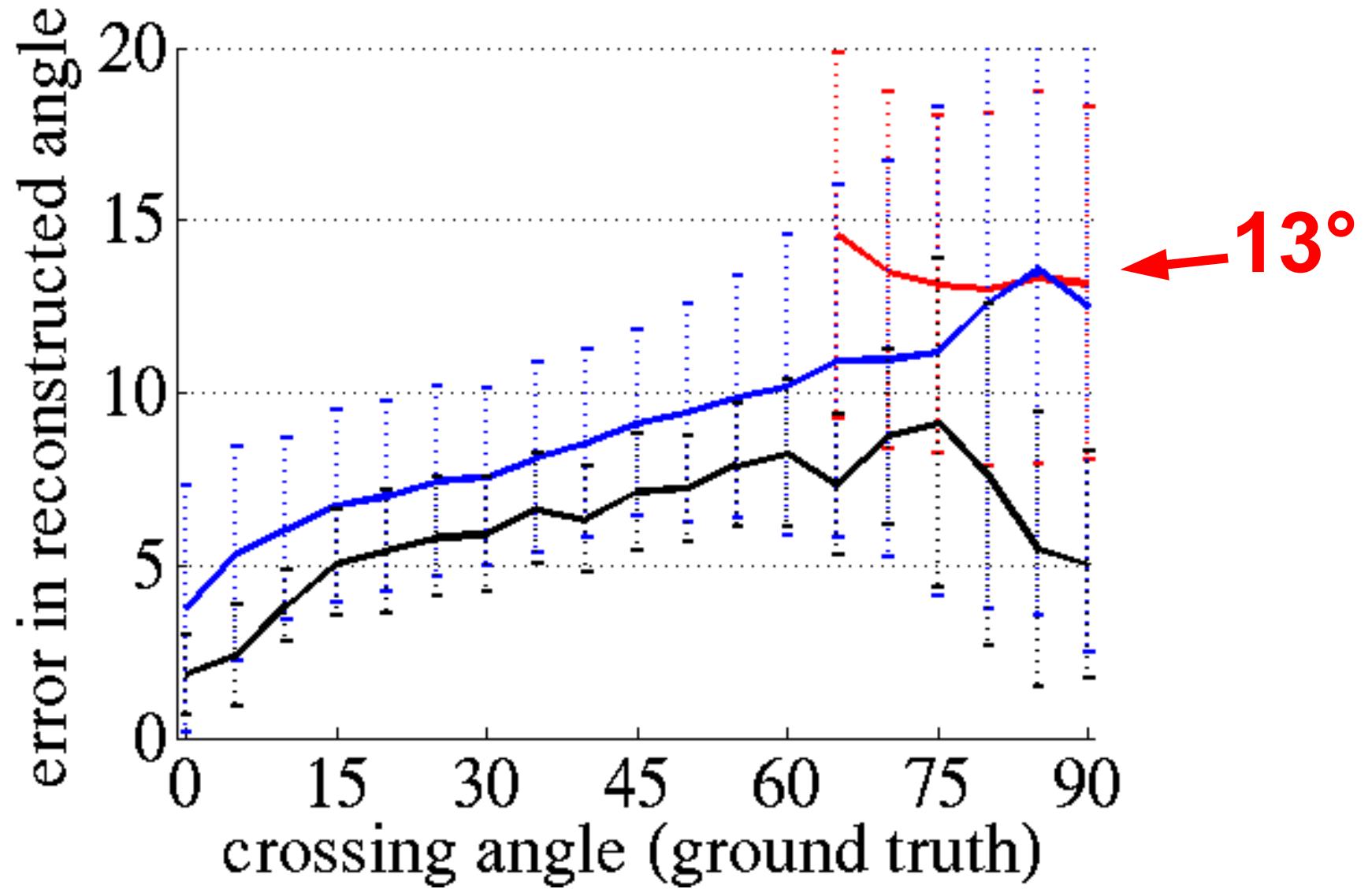
$\text{SNR} \approx 5, b = 1000$

unequal signal field: 60/40



SNR ≈ 5 , b = 1000

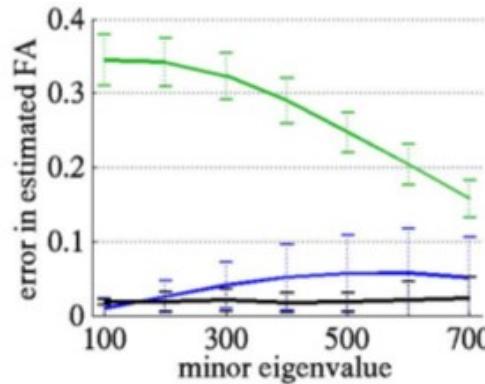
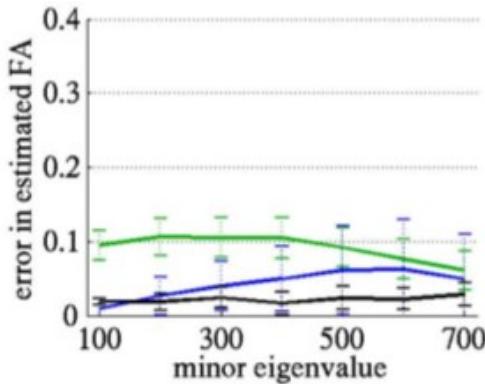
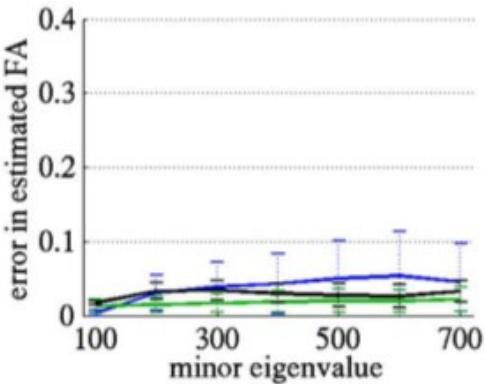
unequal signal field: 70/30



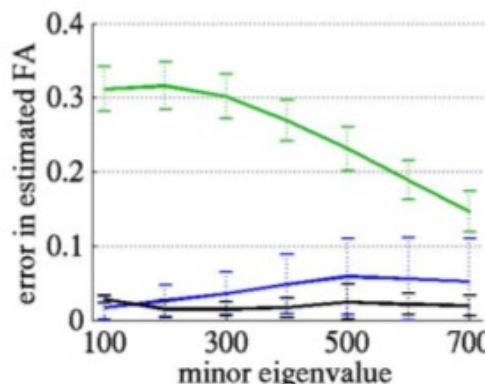
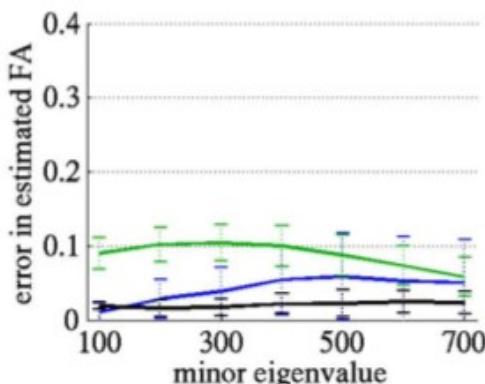
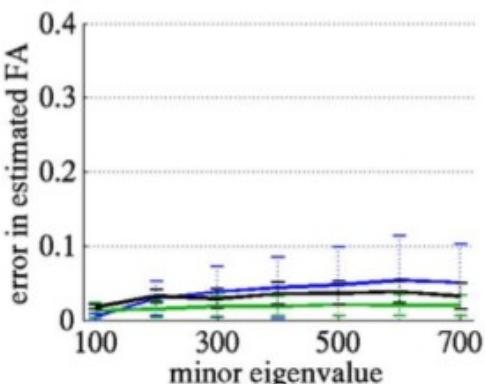
SNR ≈ 5 , b = 1000

estimation fidelity

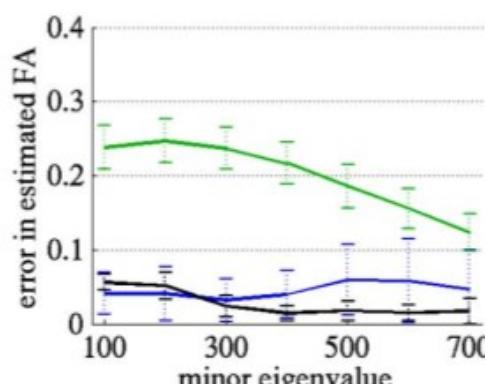
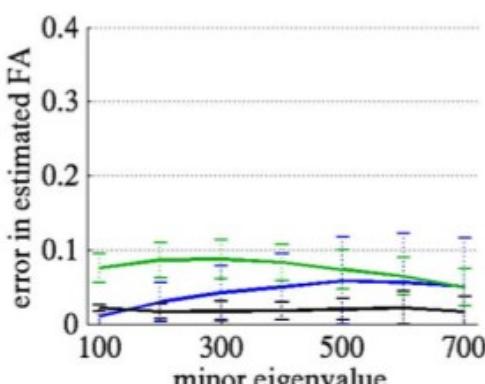
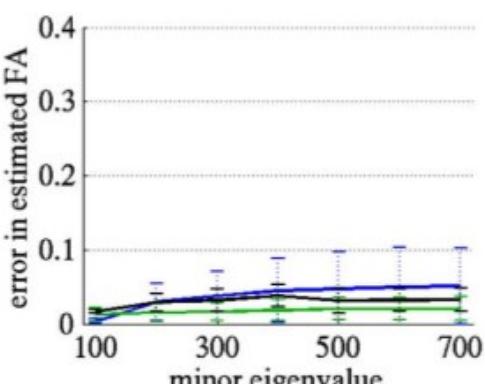
50/50



60/40



70/30



one fiber
(no crossing)

45 degree crossing

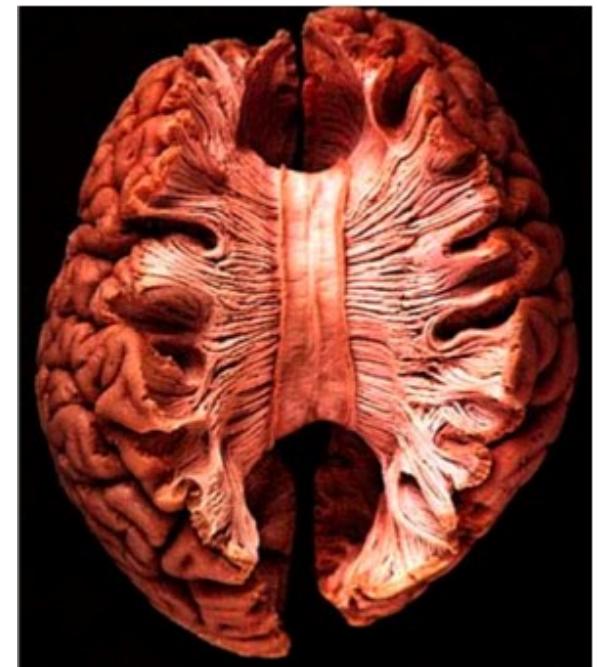
90 degree crossing



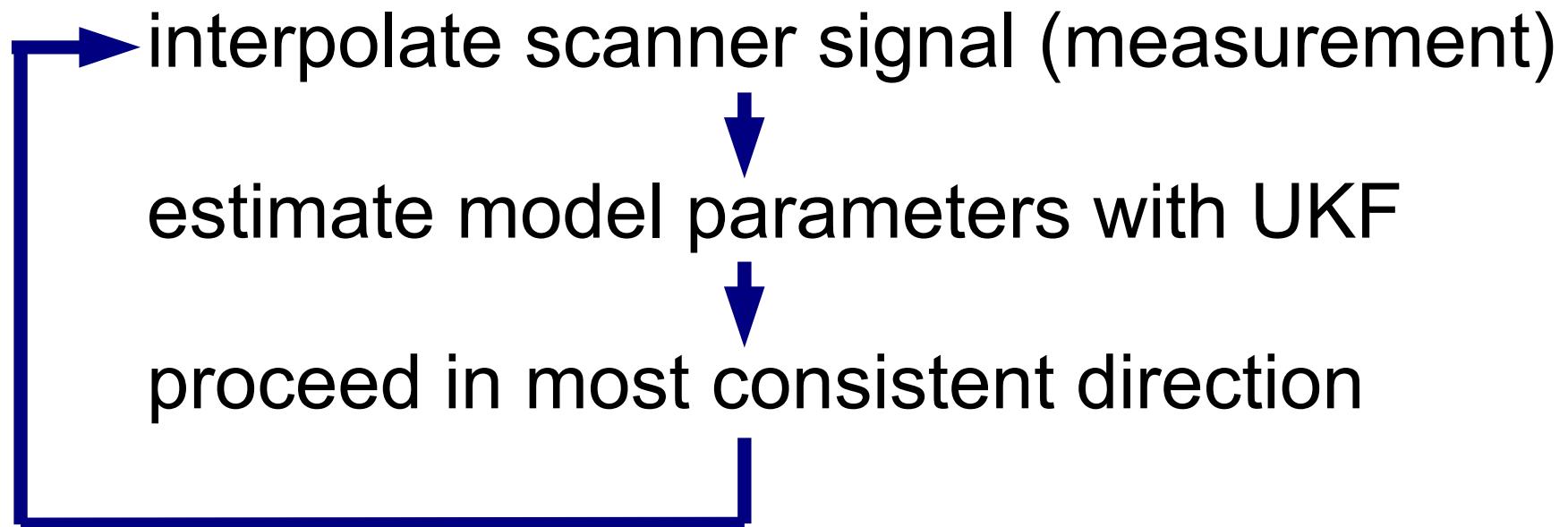
in vivo



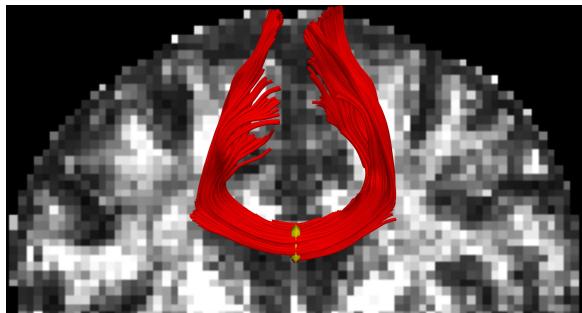
b=900
51 directions
1.7mm isotropic voxel
17 minute scan



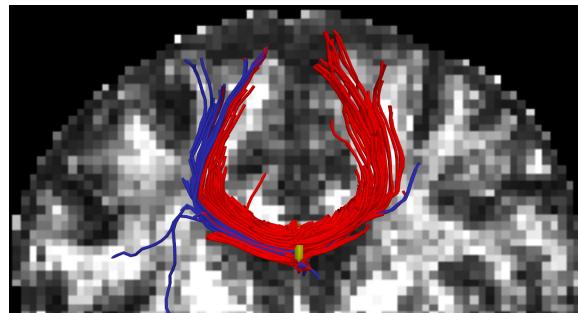
algorithm



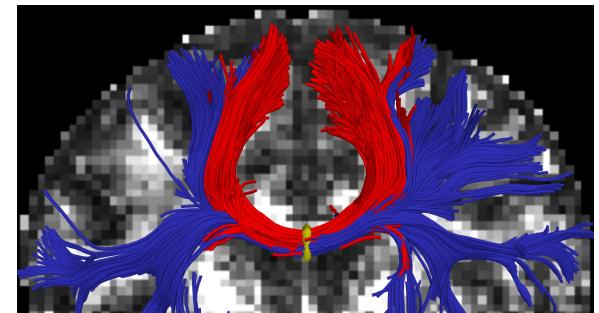
terminate: $FA < 0.15$



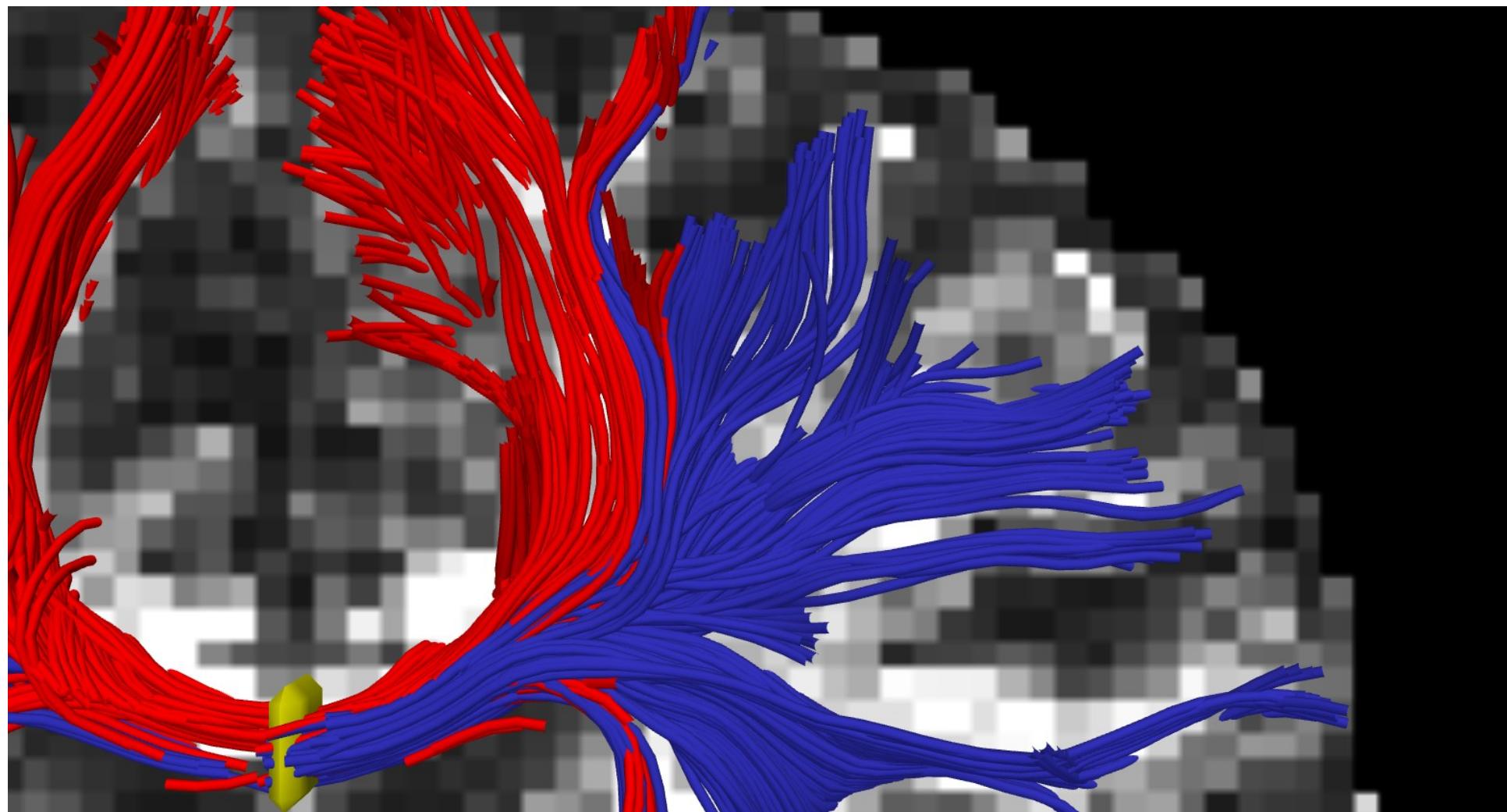
single tensor



spherical harmonics



filtered two-tensor

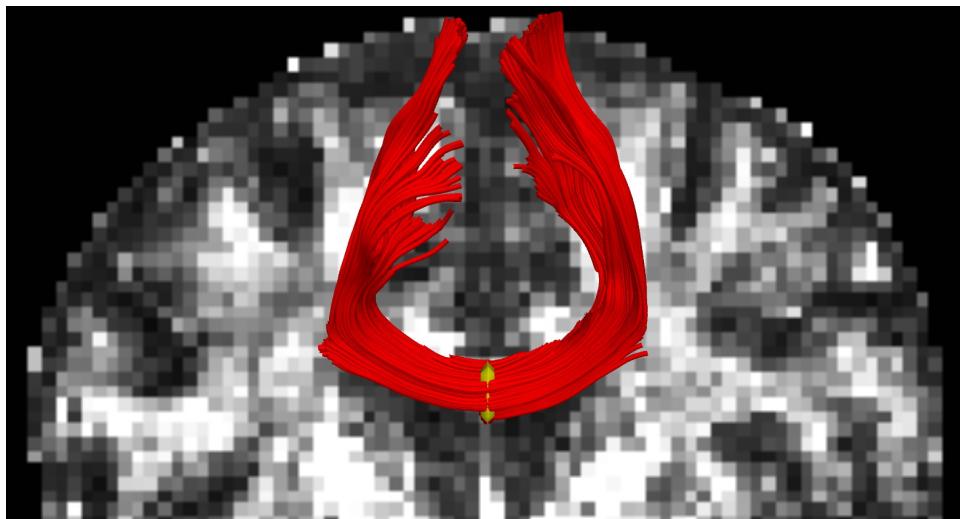


filtered two-tensor

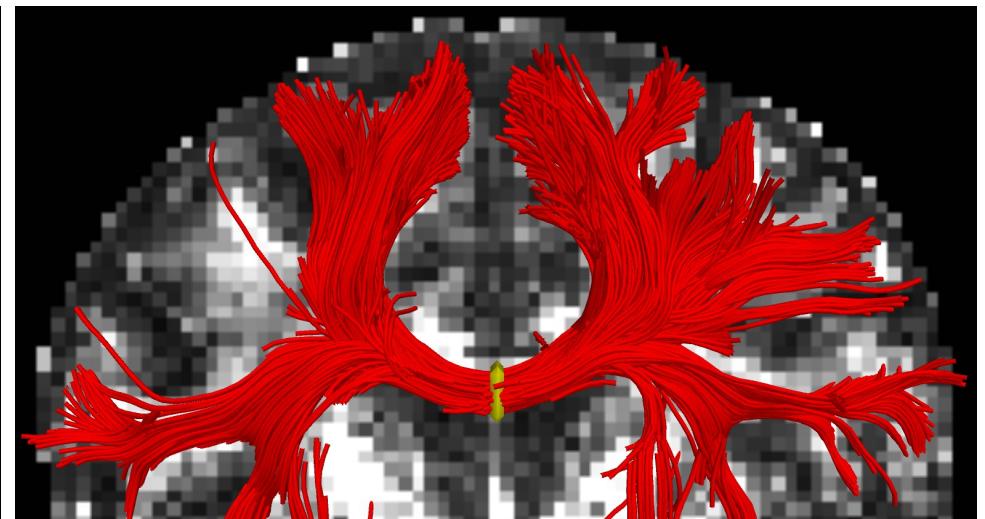
($b = 900$, 1.7mm, 51 directions)

fitting the local fiber model

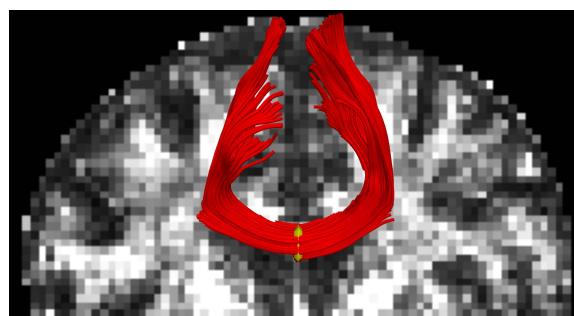
- Independent optimization v. filtered estimation
- Nonlinear model: Unscented Kalman filter



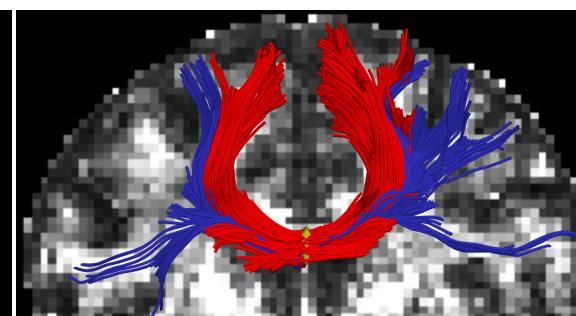
single-tensor



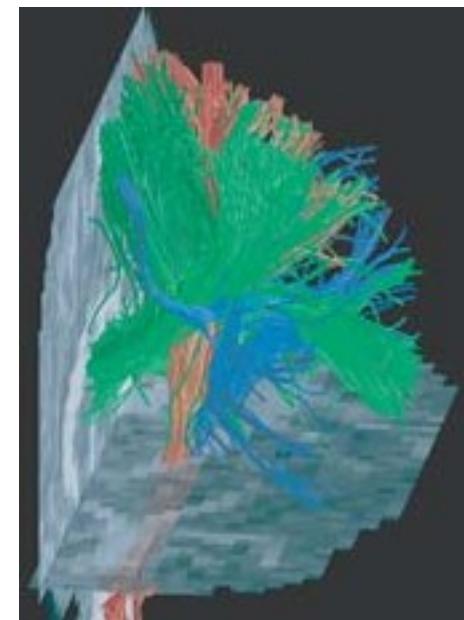
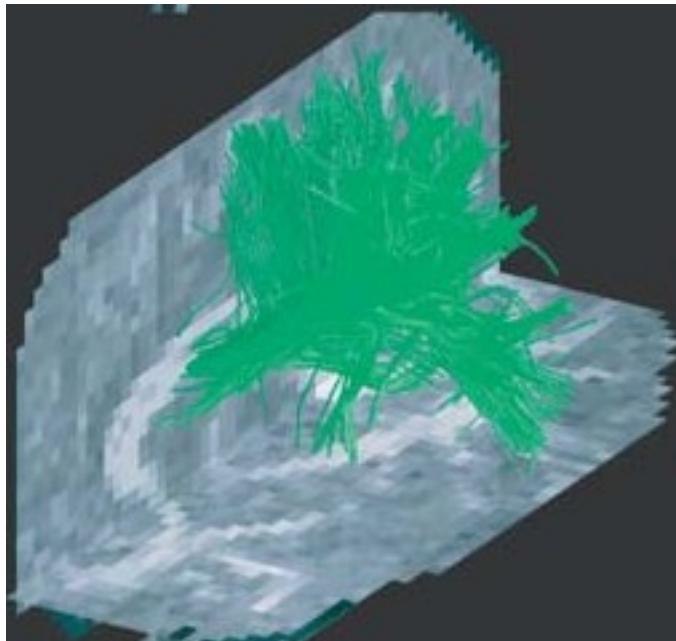
filtered two-tensor



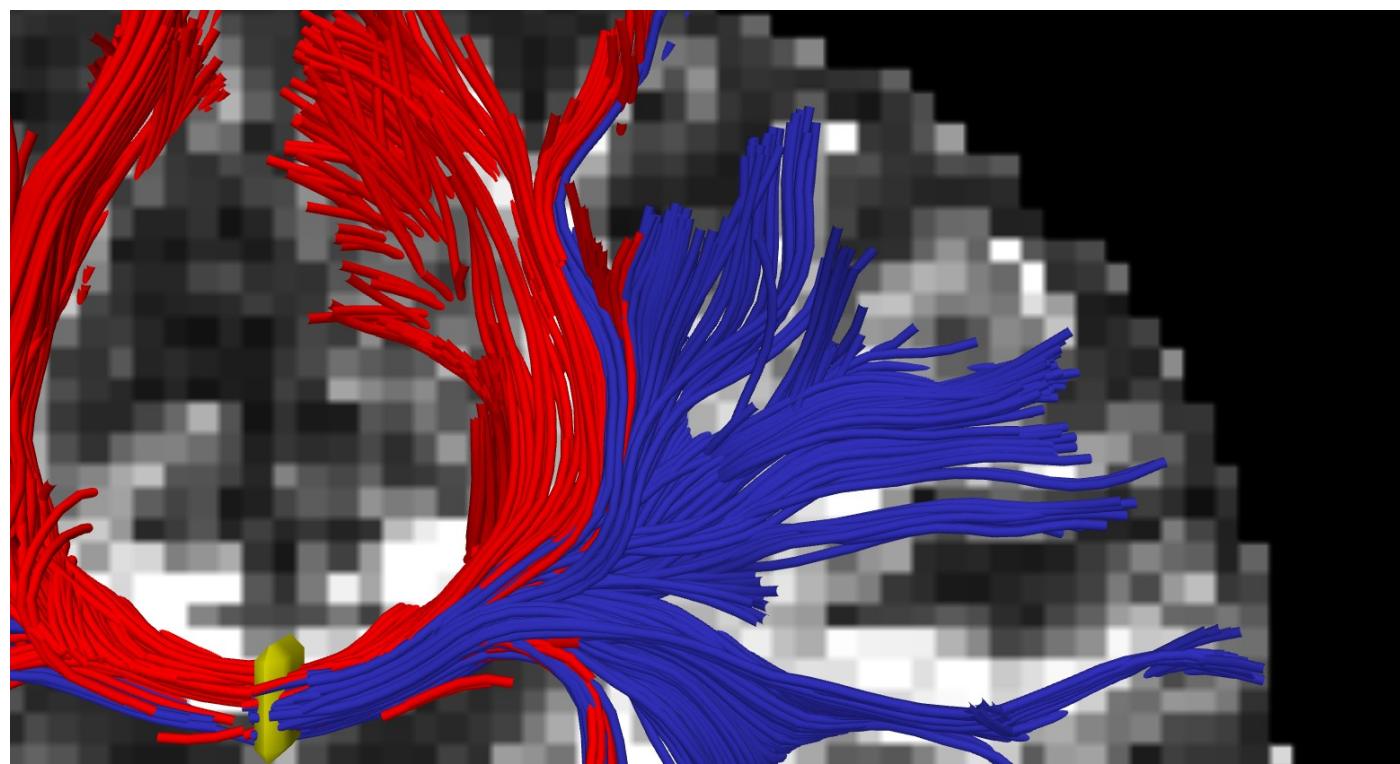
single tensor



filtered two-tensor

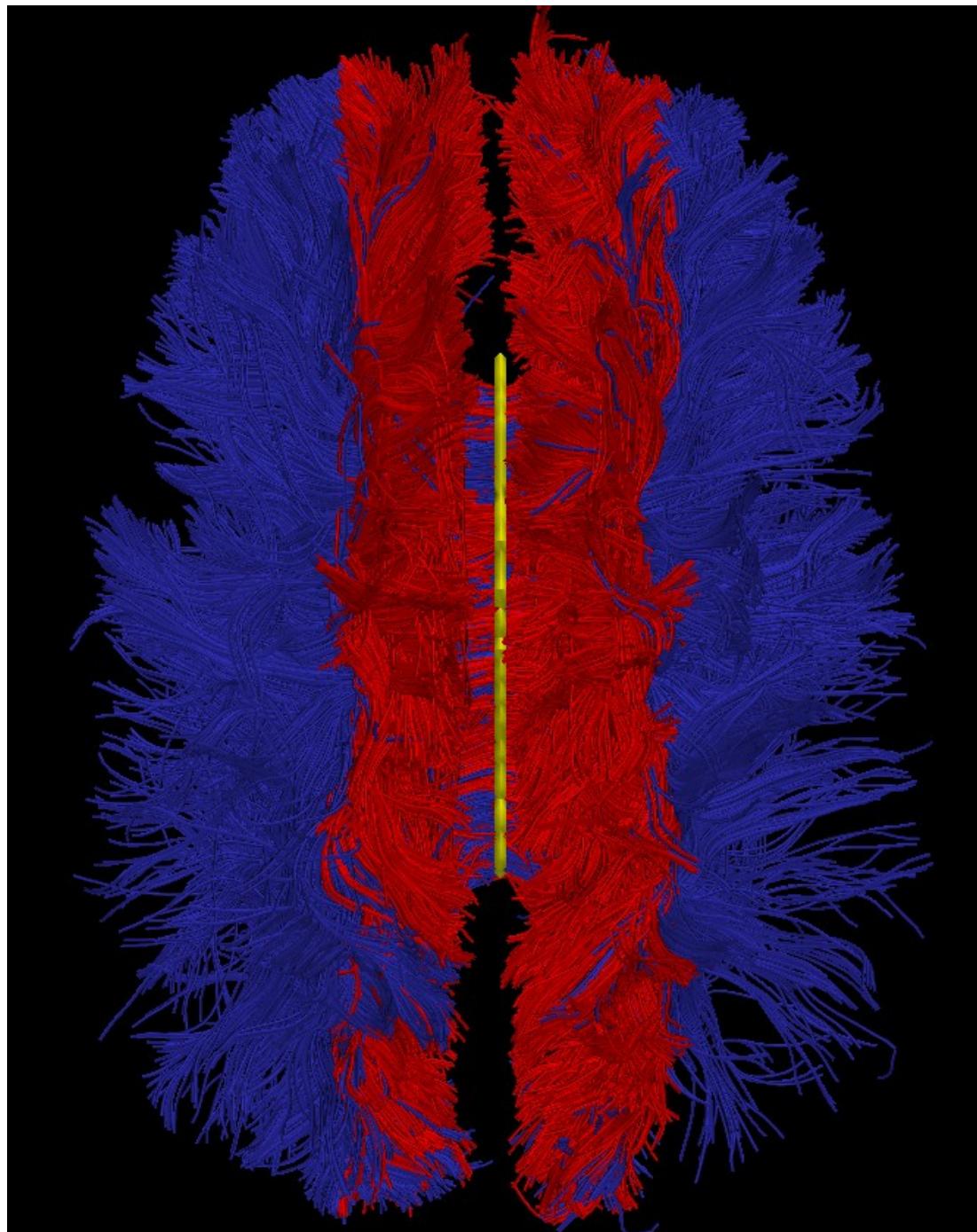


DSI [Hagmann 05]



filtered two-tensor

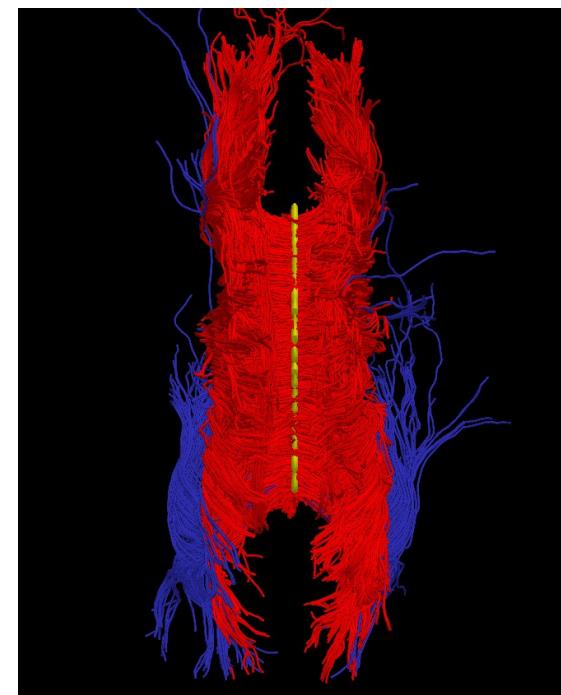




filtered two-tensor



single tensor

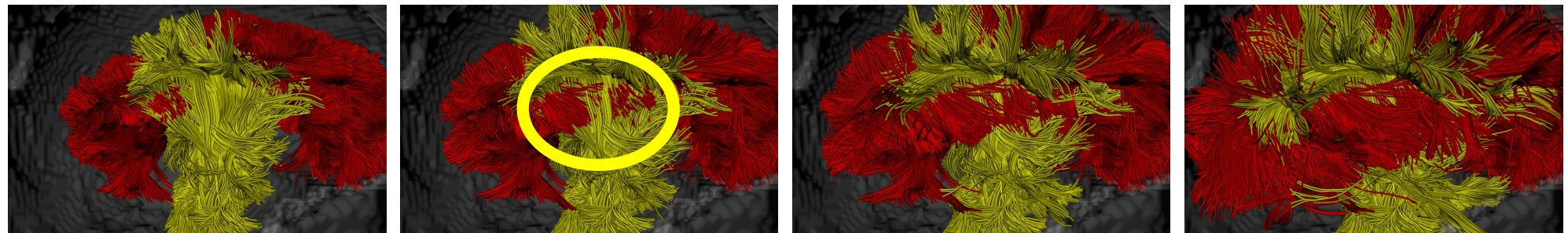


spherical harmonics

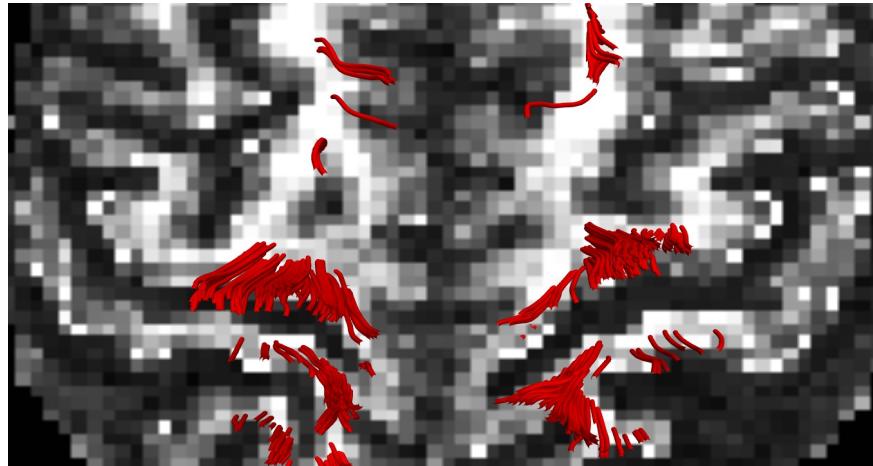


corpus callosum

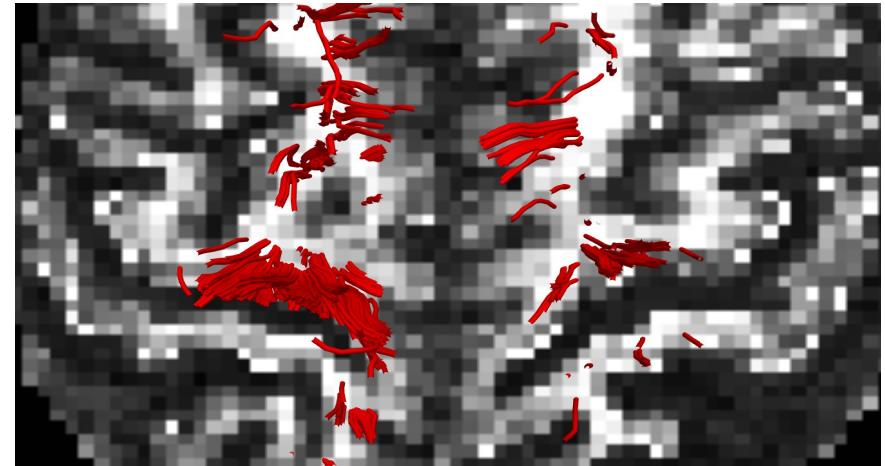
internal capsule



centrum semiovale



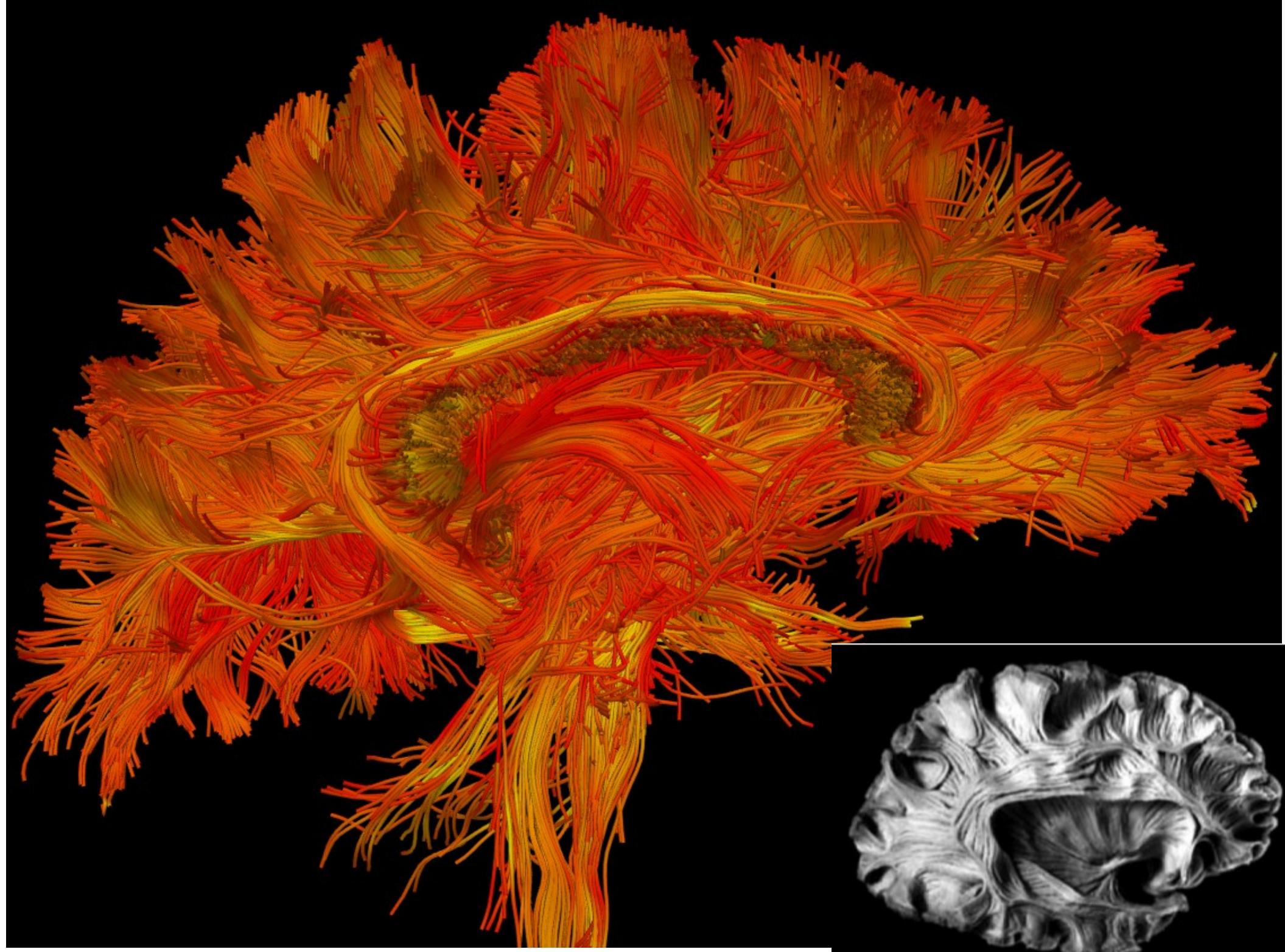
single tensor



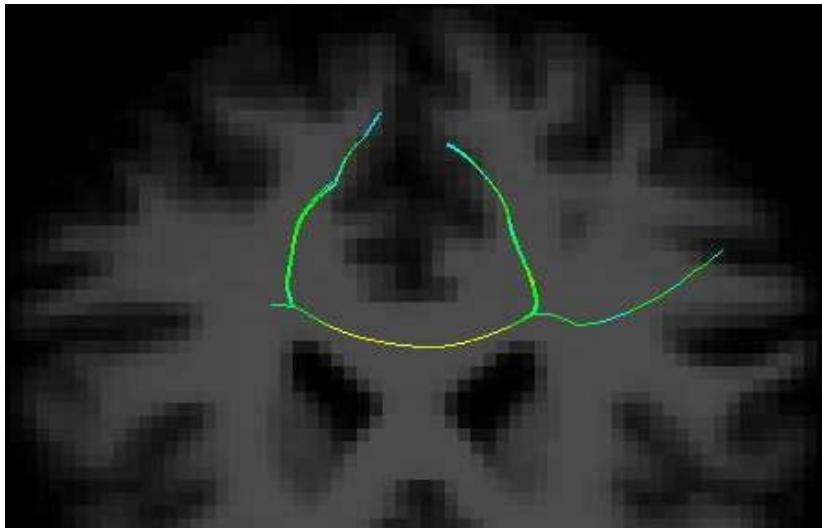
spherical harmonics



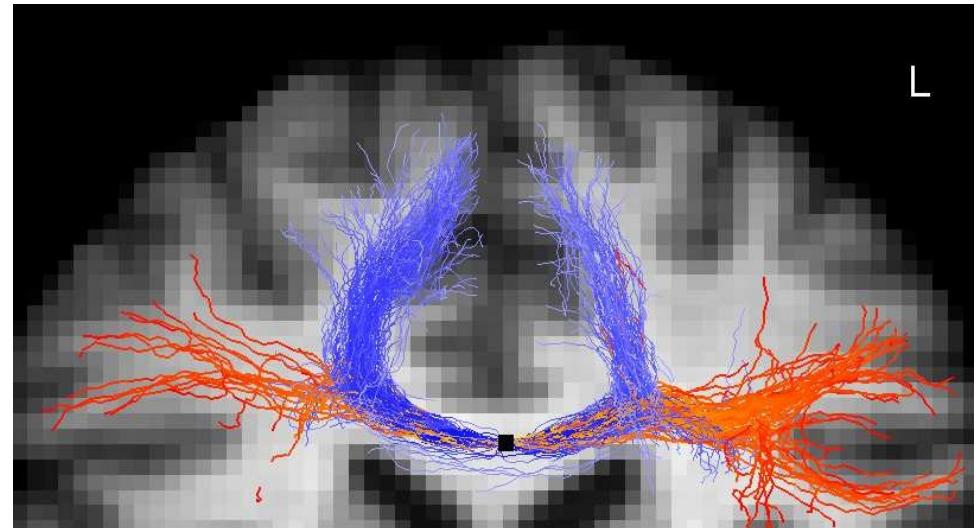
filtered two-tensor



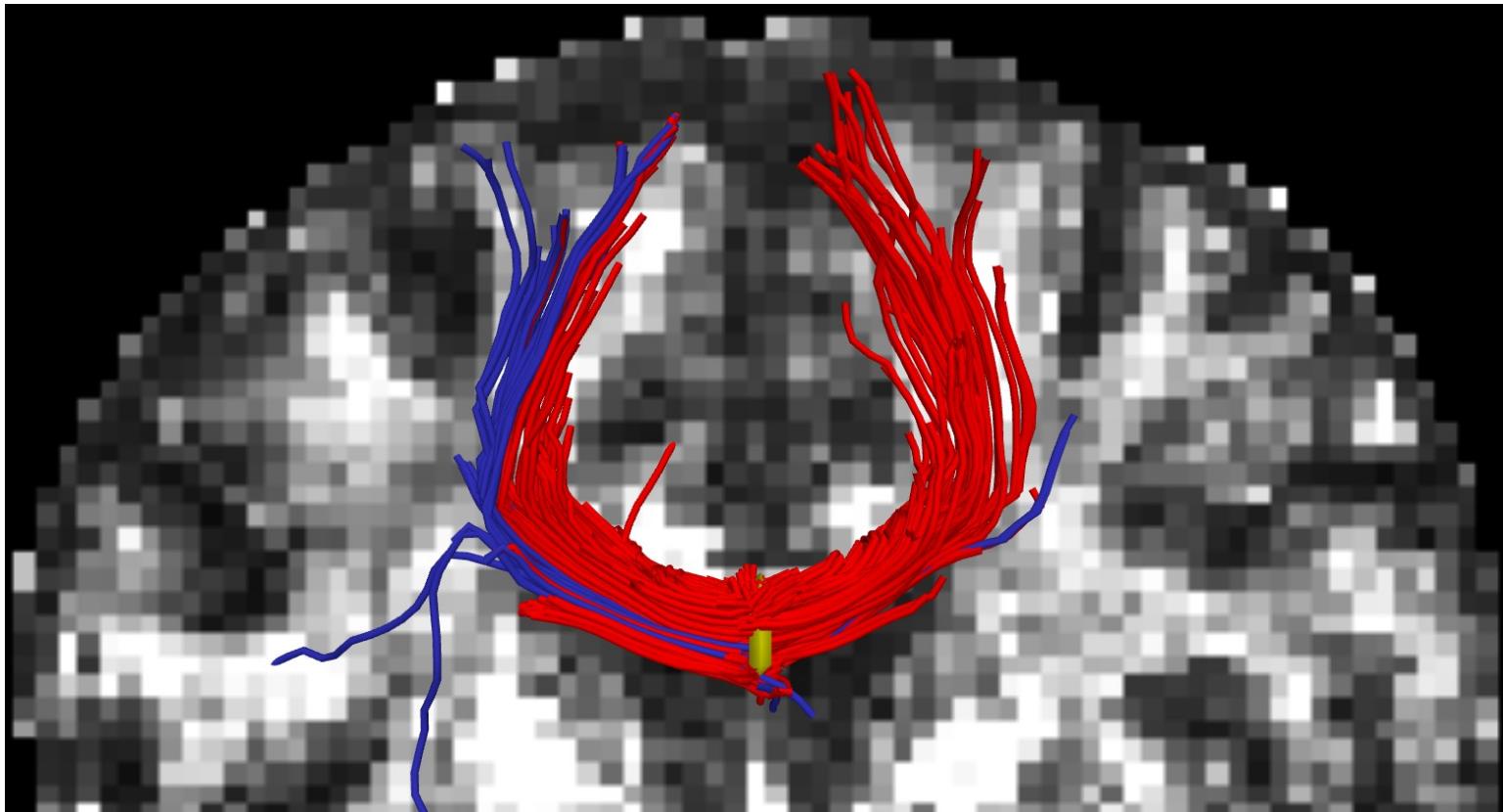
related work



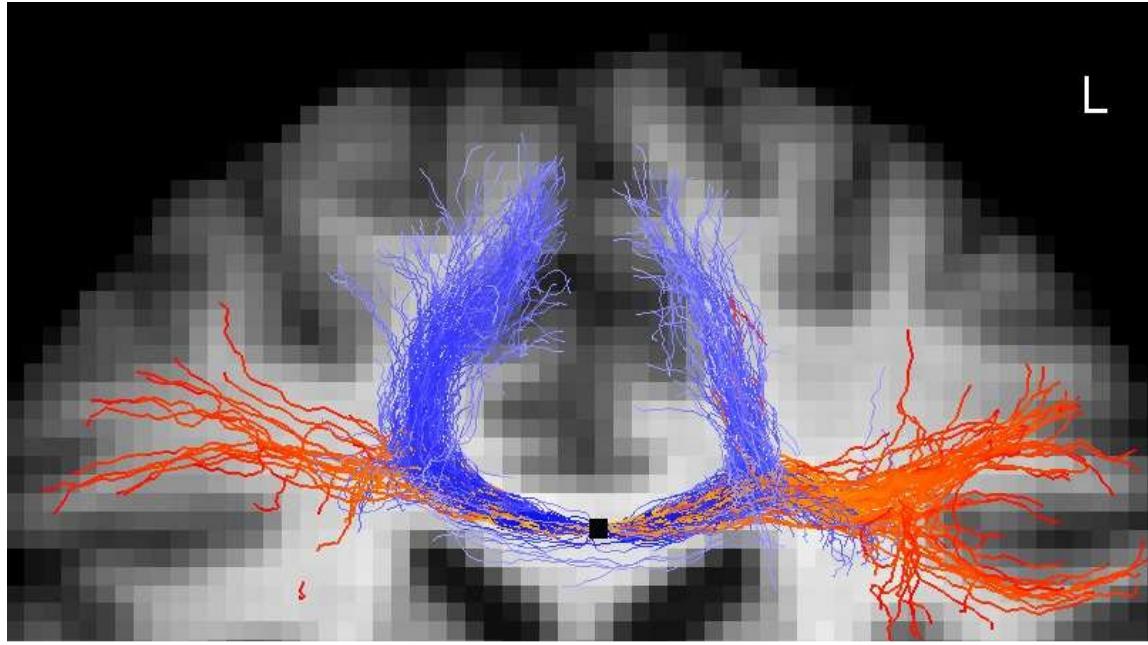
Deterministic (Descoteaux 2007)



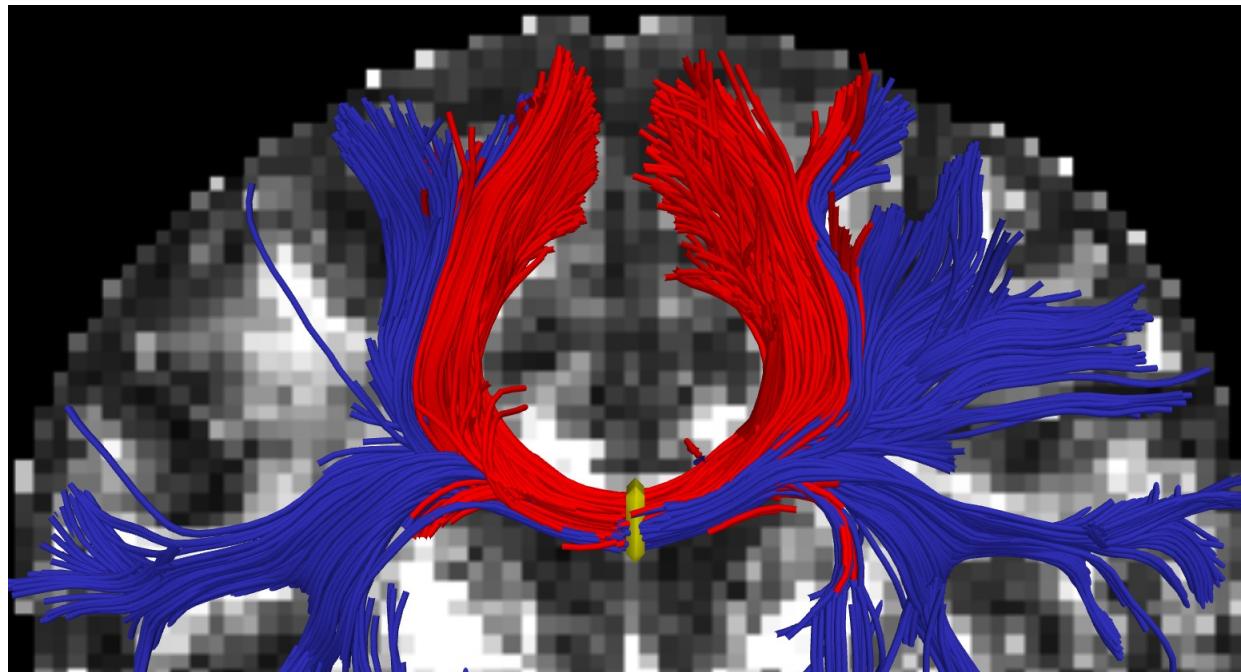
Probabilistic (Descoteaux 2007)



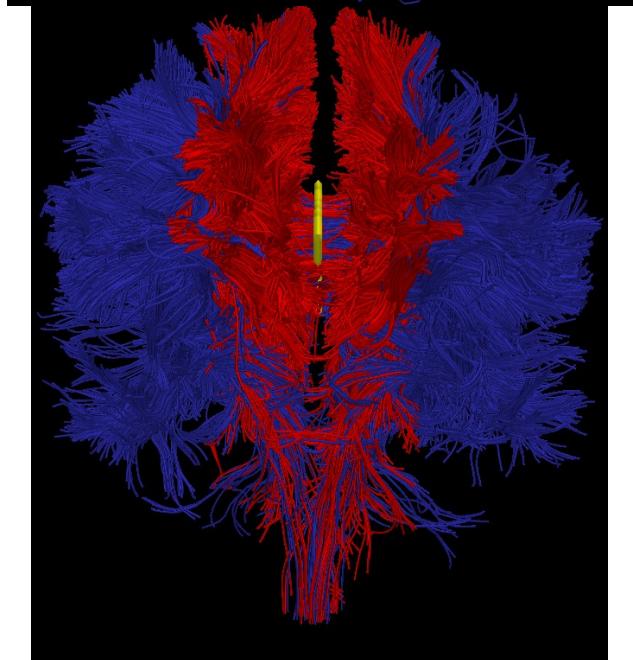
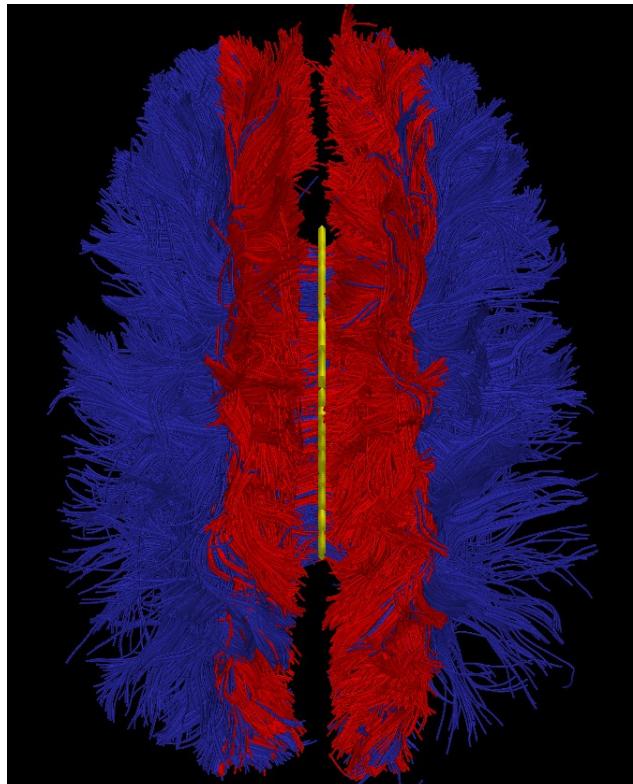
our implementation of spherical harmonics



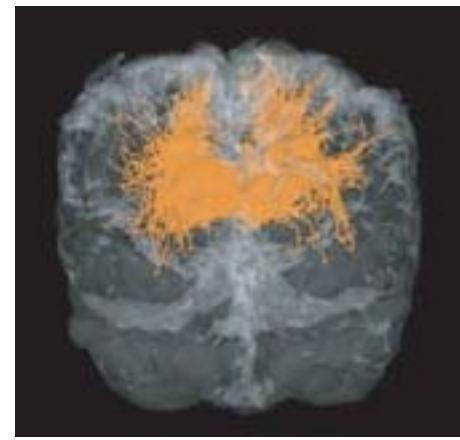
spherical harmonics, **probabilistic** tractography
[Descoteaux 2007]



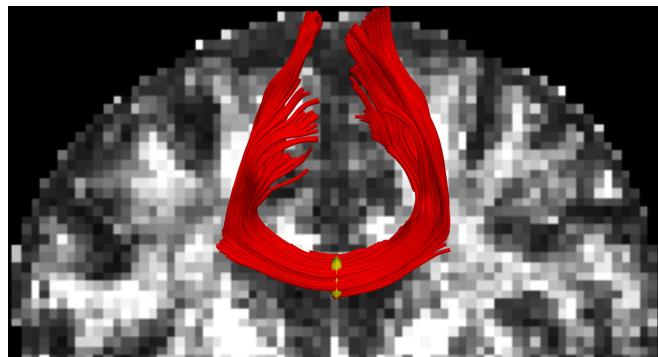
filtered two-tensor, **deterministic** tractography



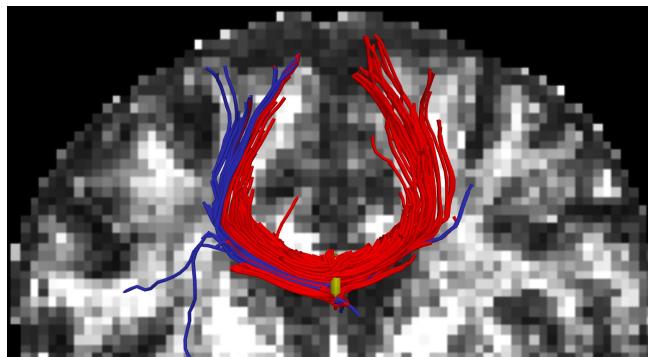
filtered two-tensor



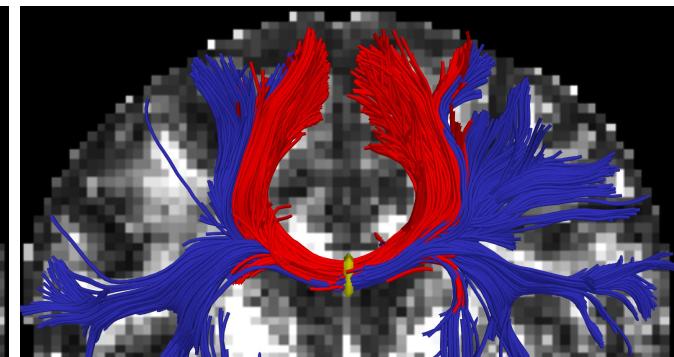
DSI [Hagmann 2005]



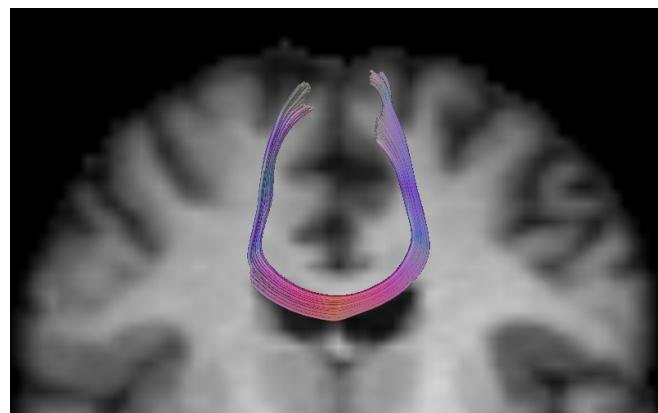
single tensor streamline



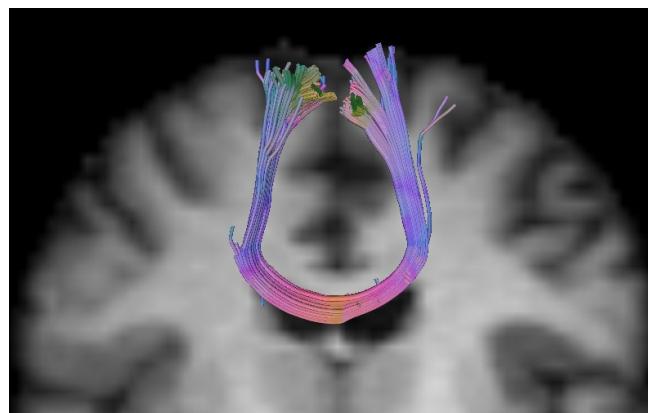
spherical harmonics



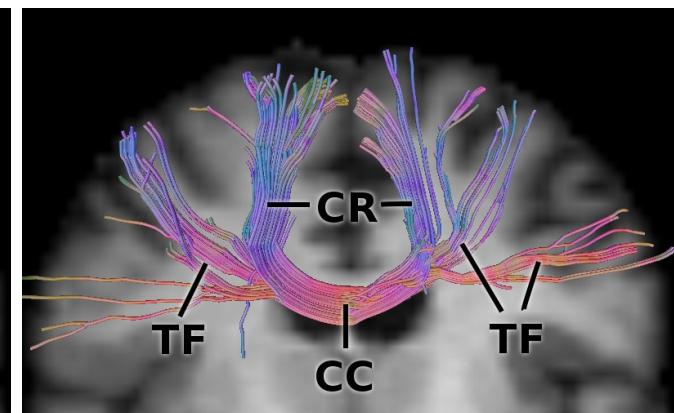
filtered two-tensor



single tensor streamline



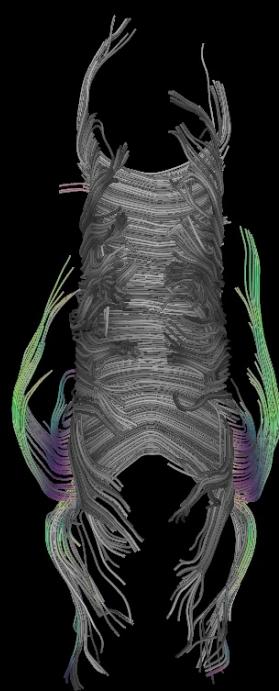
peak detection
(our “spherical harmonics”)



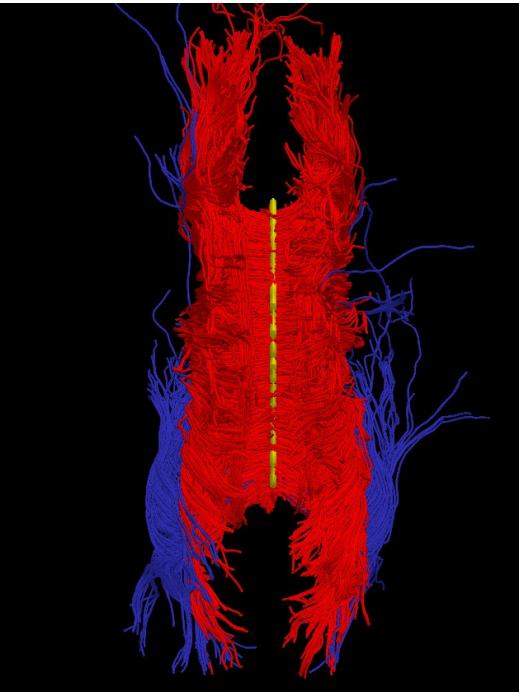
tensor decomposition

[Schultz 2008]

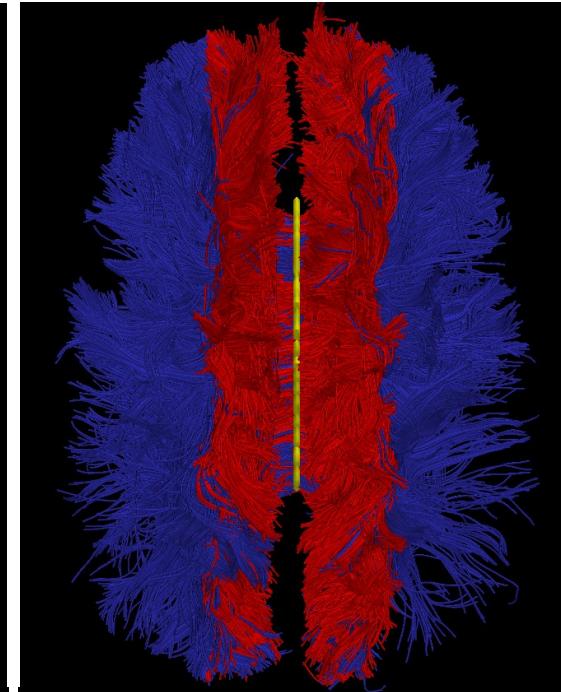
filtered two-tensor



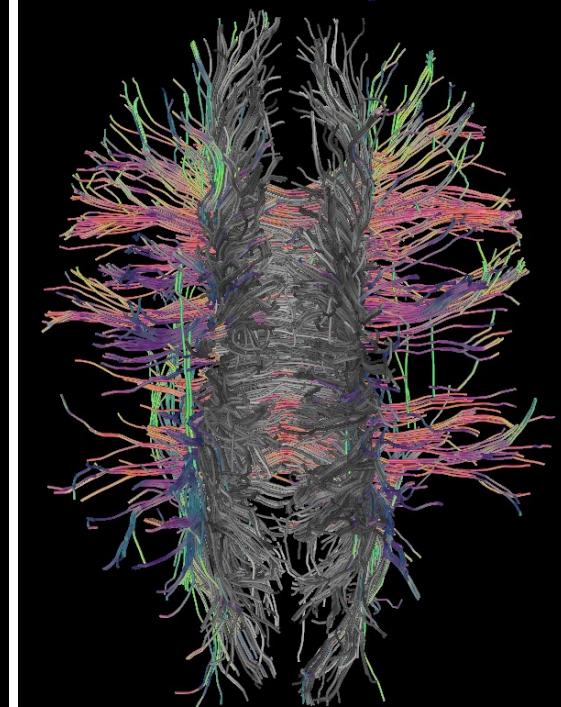
single tensor

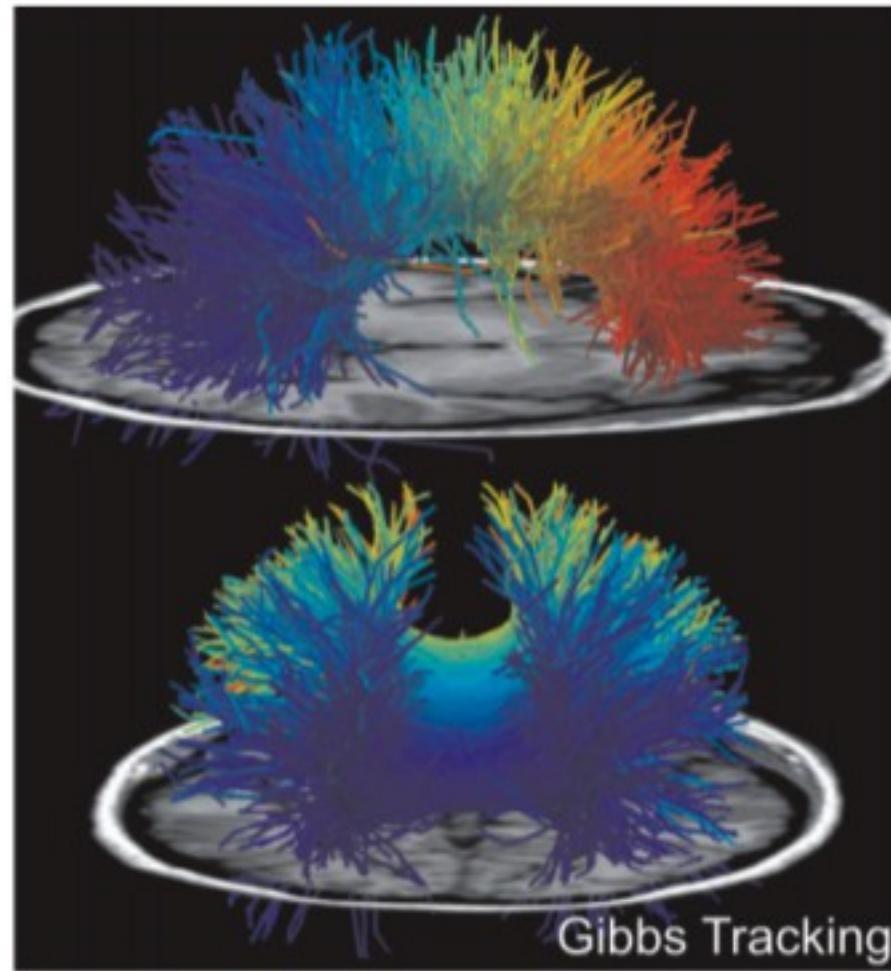


spherical harmonics



tensor decomposition
[Schultz 2008]





[Kreher 08]

~1 month to compute

conclusion

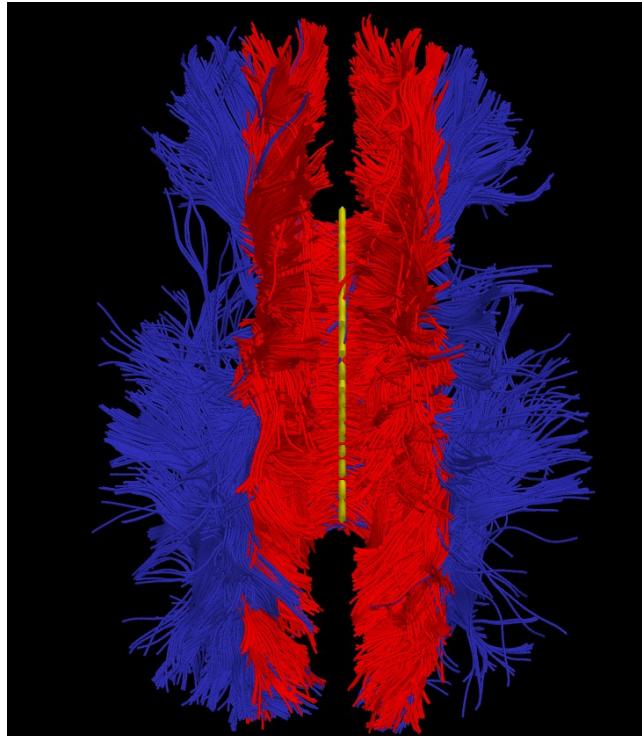
inherent coherence along the fiber

we should exploit it in the estimation

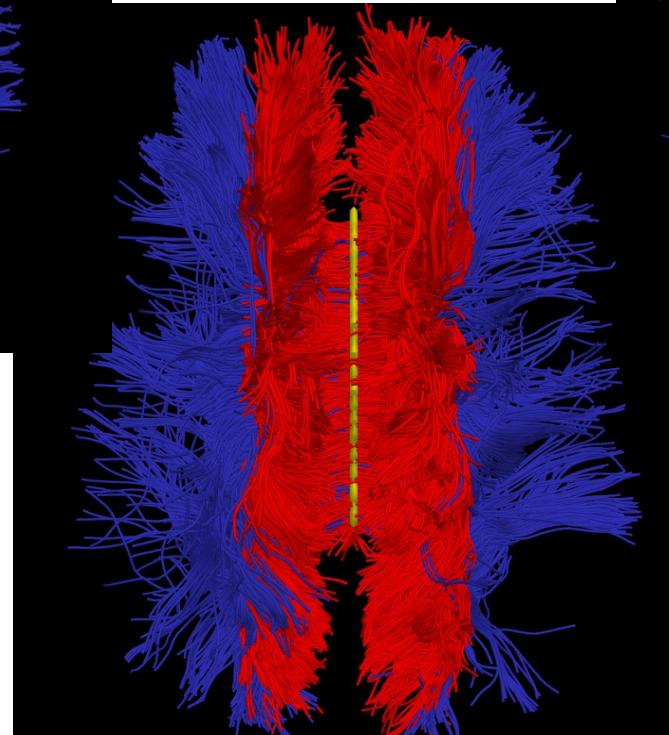
from the proposal...

- tensors: IPMI 2009, TMI 2010
- weighted mixtures: MICCAI 2009
- validation (phantom): DMFC (MICCAI) 2010
- Slicer3 module: Slicer 3.6 (?)
- population study: DMFC (MICCAI) 2010
- local voxel model, global path model: MICCAI 2010

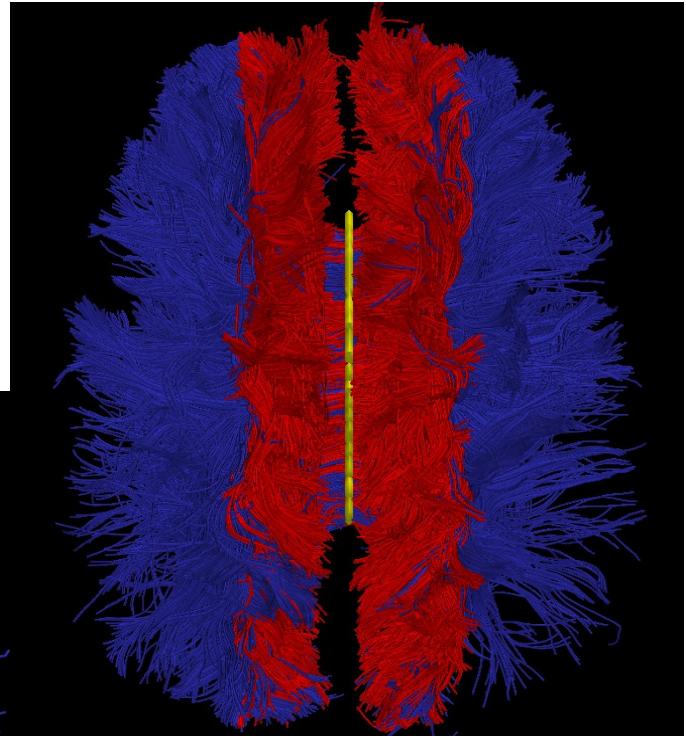
variations



Watson functions



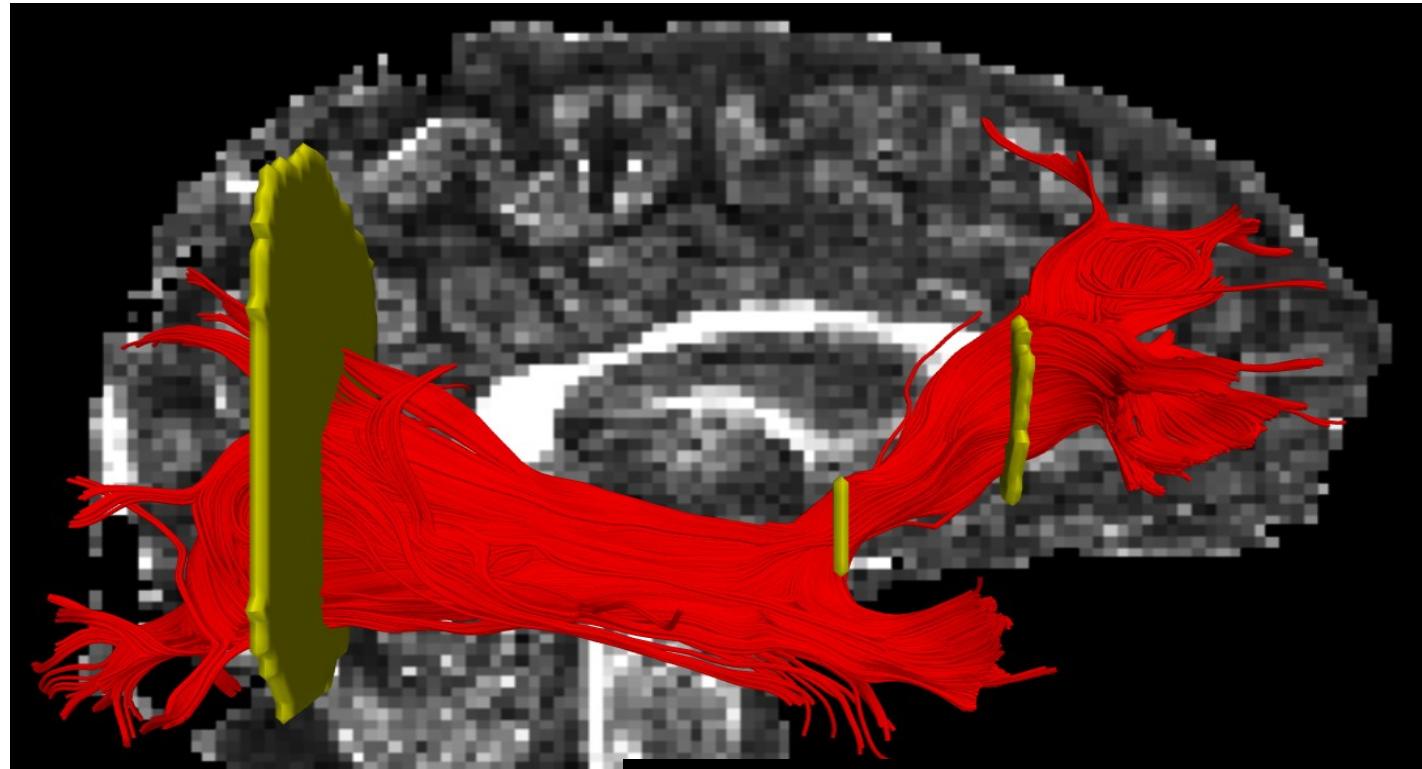
weighted models



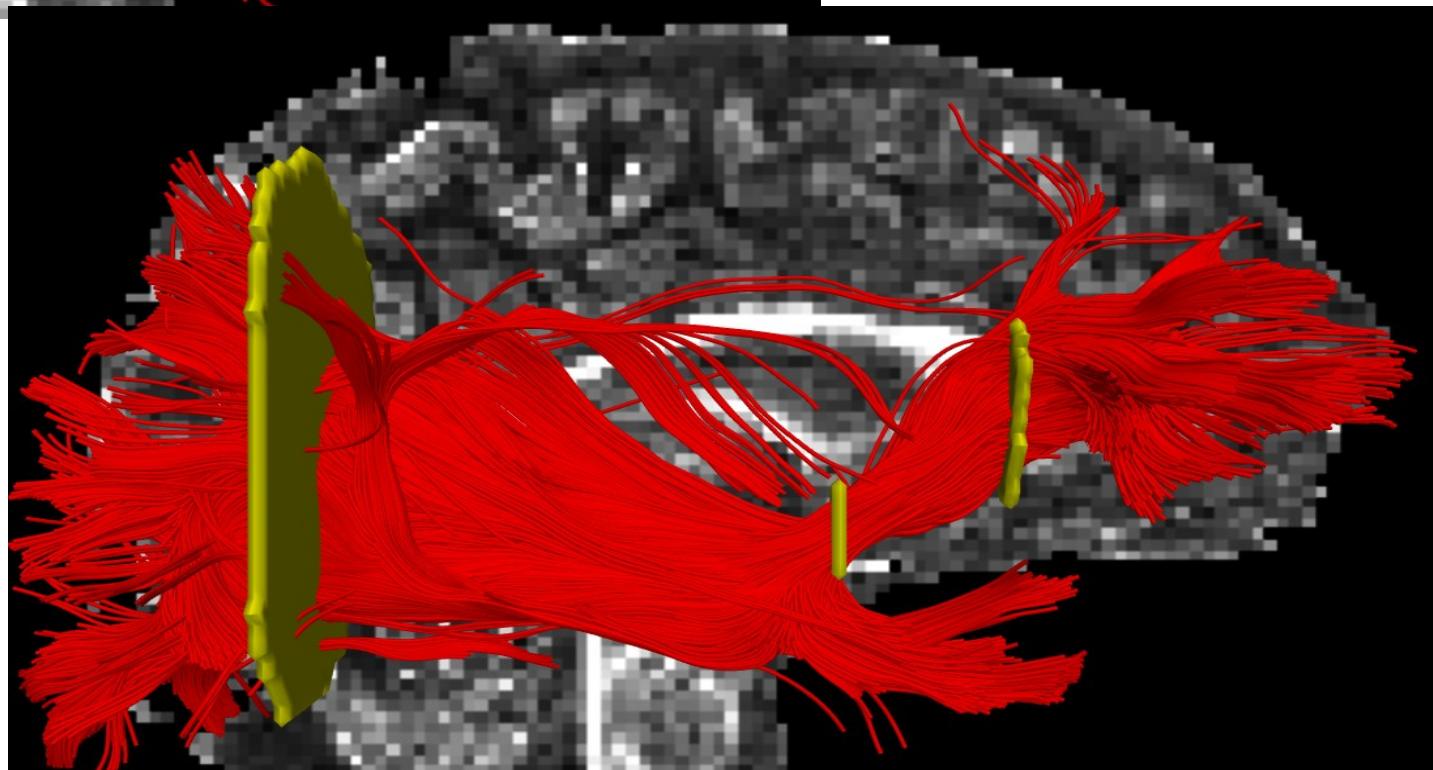
tensors

parametric:
mixture models
non-parametric:
spherical harmonics
higher-order
tensors

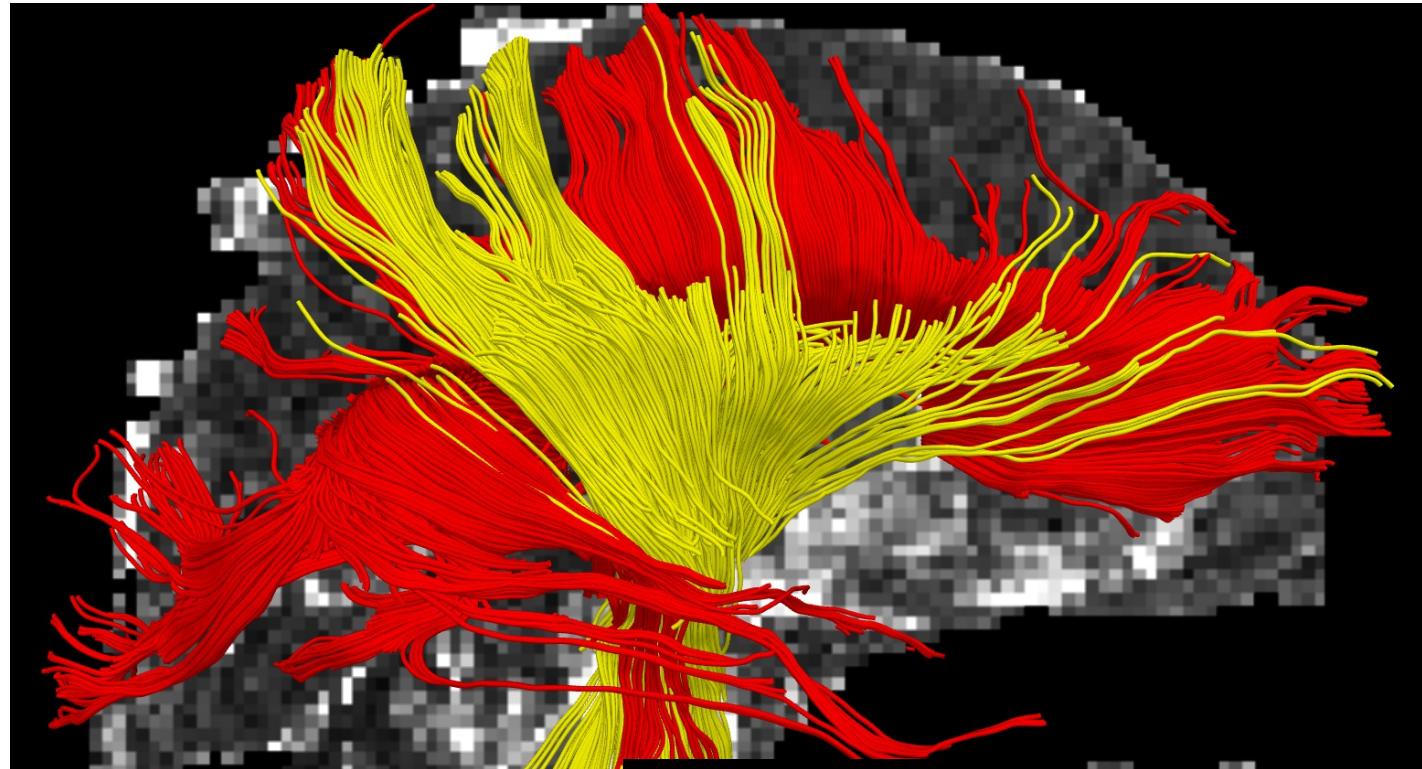
Malcolm, Shenton, Rathi. Two-tensor tractography using a constrained filter. In MICCAI, p.894–902, 2009.
Rathi, Malcolm, Michailovich, Westin, Shenton, Bouix. Tensor-kernels for simultaneous fiber model estimation and tractography. *Magnetic Resonance in Medicine*, 64(1):138–148, 2010.



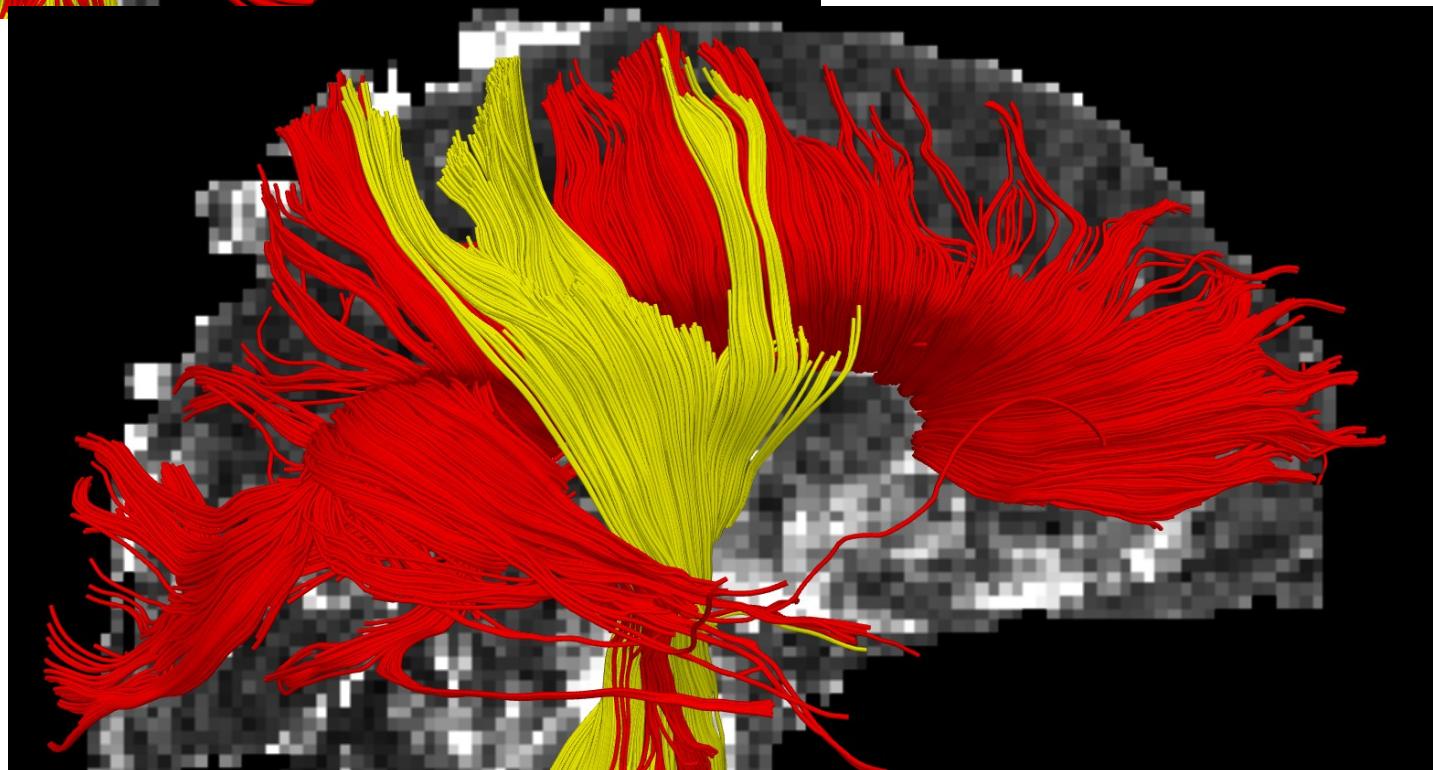
streamline
single-tensor



filtered
single-tensor



streamline
single-tensor



filtered
single-tensor

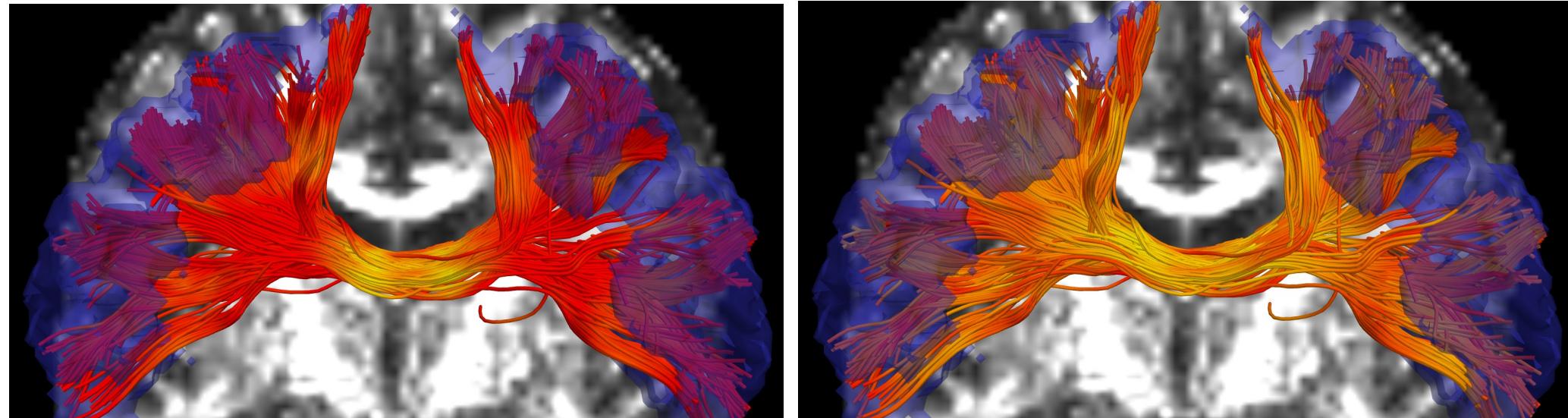
model components one or two?

a population study

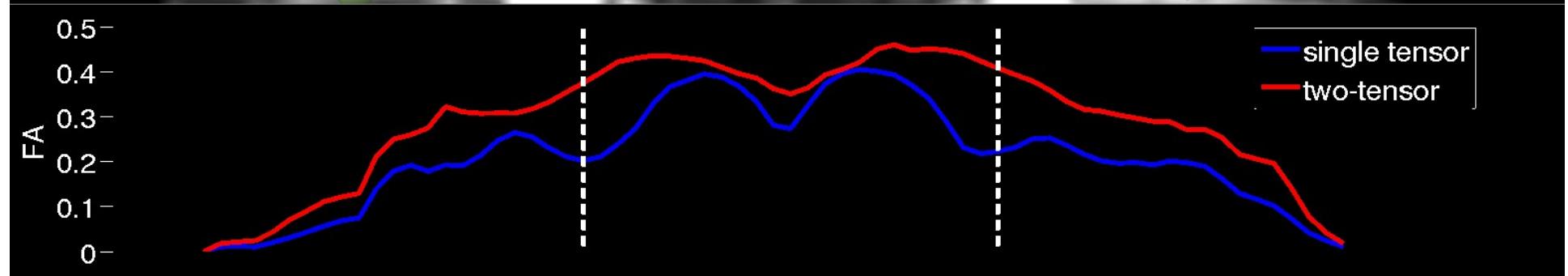
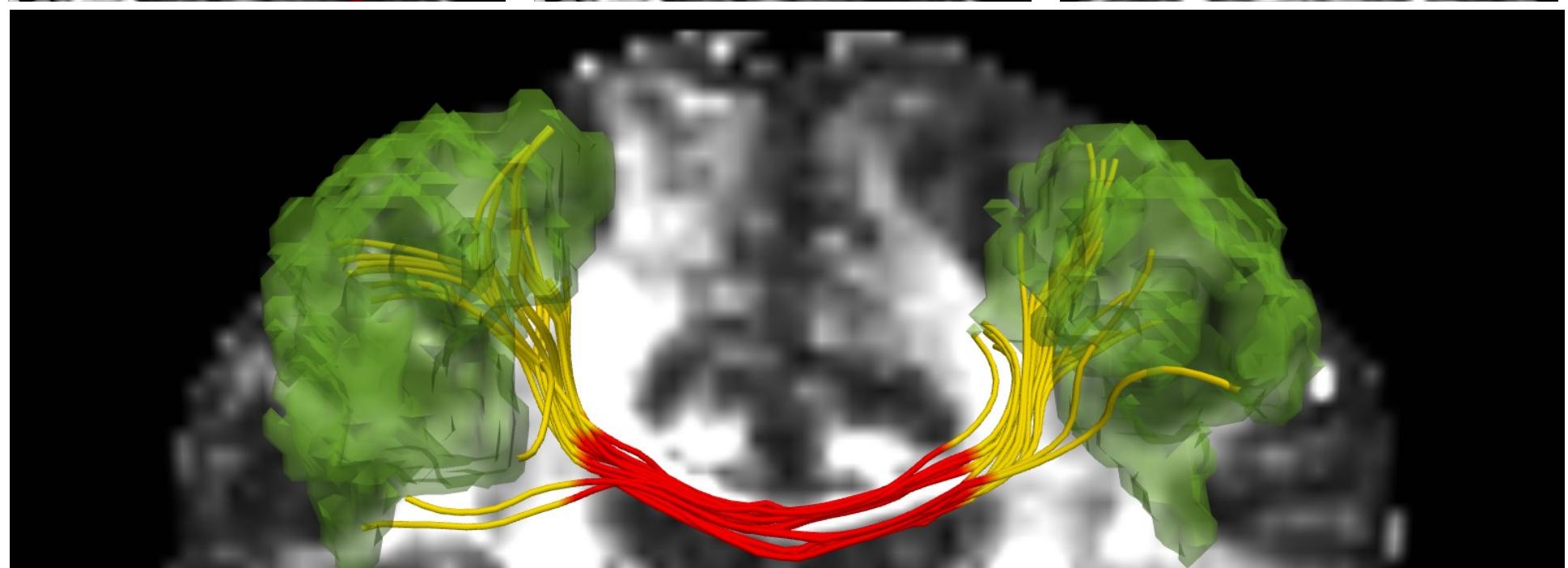
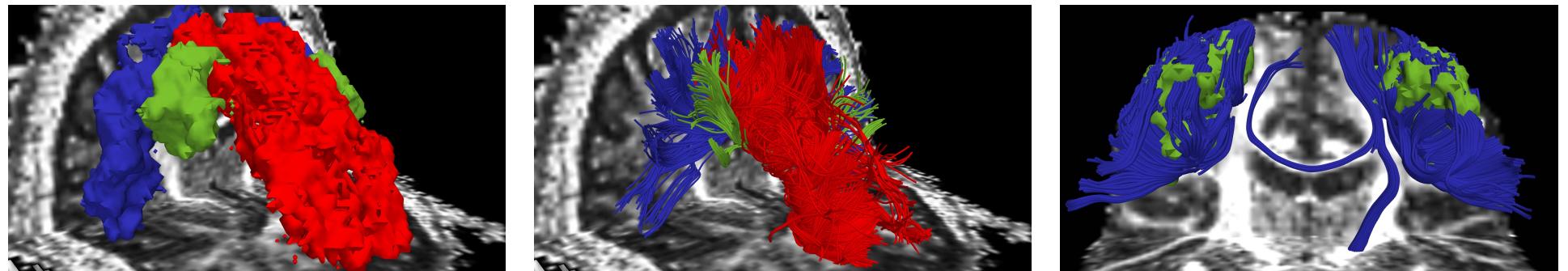
Malcolm, Kubicki, Shenton, Rathi. The effect of local fiber model on population studies. In Diffusion Modeling and Fiber Cup (in MICCAI), pages 33–40, 2009.

Rathi, Malcolm, Michailovich, Goldstein, Seidman, McCarley, Westin, Shenton. Biomarkers for identifying first-episode schizophrenia patients using diffusion weighted imaging. In MICCAI, volume 6361, pages 657–665, 2010.

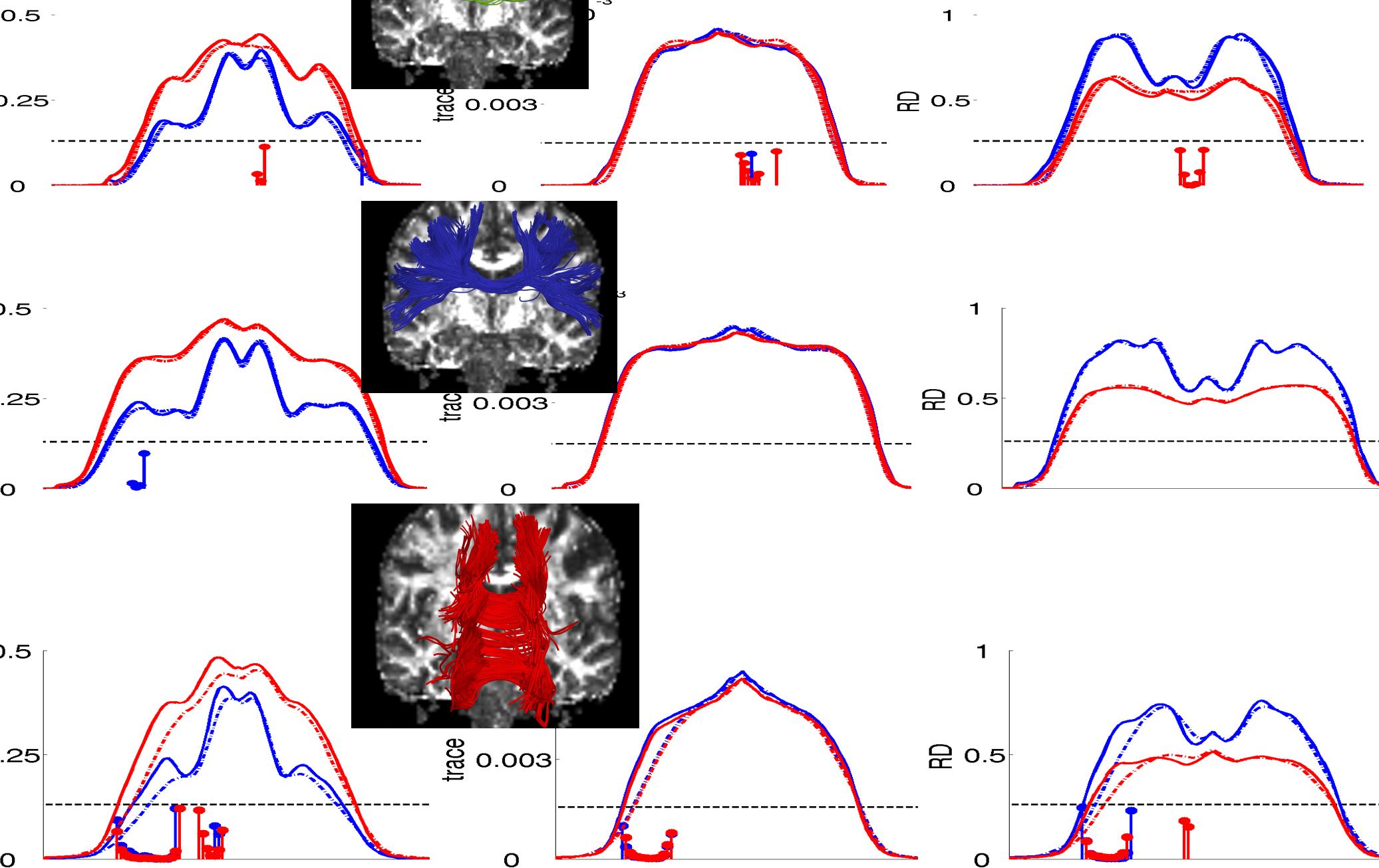
Experiment: look at FA superimposed on two-tensor fibers

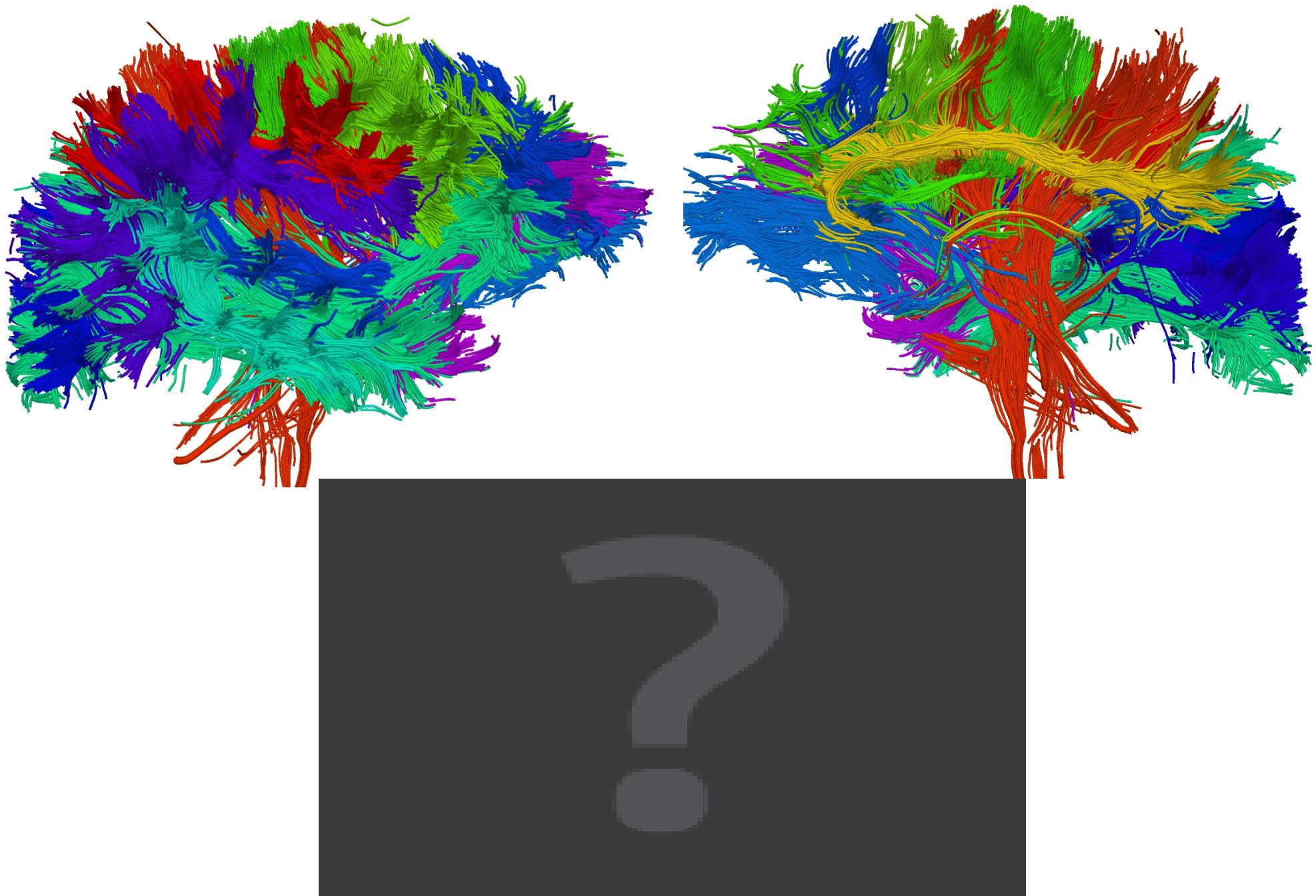


Result: single-tensor FA drops outside corpus callosum while two-tensor maintains higher FA on out to gray-matter



1T 2T





J. G. Malcolm, M. E. Shenton, and Y. Rathi. Filtered tractography: State estimation in a constrained subspace. In Diffusion Modeling and Fiber Cup (in MICCAI), pages 122–133, 2009.



end

extra...

the watson approximation

J. G. Malcolm, O. Michailovich, S. Bouix, C.-F. Westin, M. E. Shenton, and Y. Rathi. A filtered approach to neural tractography using the Watson directional function. *Medical Image Analysis*, 14:58–69, 2010.

do we need six parameters?

- for tractography, care most about direction
 - 3 parameters
- approximate diffusivity with scalar anisotropy
 - fractional anisotropy
 - 1 parameter

Watson approximation

$$S(\mathbf{u}) = s_0 e^{-b\mathbf{u}^T D \mathbf{u}}$$

$$\begin{aligned}-b\mathbf{u}^T D \mathbf{u} &\approx -b\lambda_1 \mathbf{u}^T (\mathbf{m} \mathbf{m}^T) \mathbf{u} \\&= -b\lambda_1 (\mathbf{u}^T \mathbf{m})(\mathbf{m}^T \mathbf{u}) \\&= -k (\mathbf{u}^T \mathbf{m})^2\end{aligned}$$

$$S(\mathbf{u}) = e^{-k(\mathbf{u}^T \mathbf{m})^2}$$

principal direction $\mathbf{m} \in \mathbb{R}^3$

scaling factor $k \in \mathbb{R}$

4 parameters

[Rathi 09, Malcolm 10]

model parameters

for two fibers...

...two principal directions $m \in \mathbb{R}^3$

...two scaling factors $k \in \mathbb{R}$

4 + 4 = 8 parameters

model parameters

for two fibers...

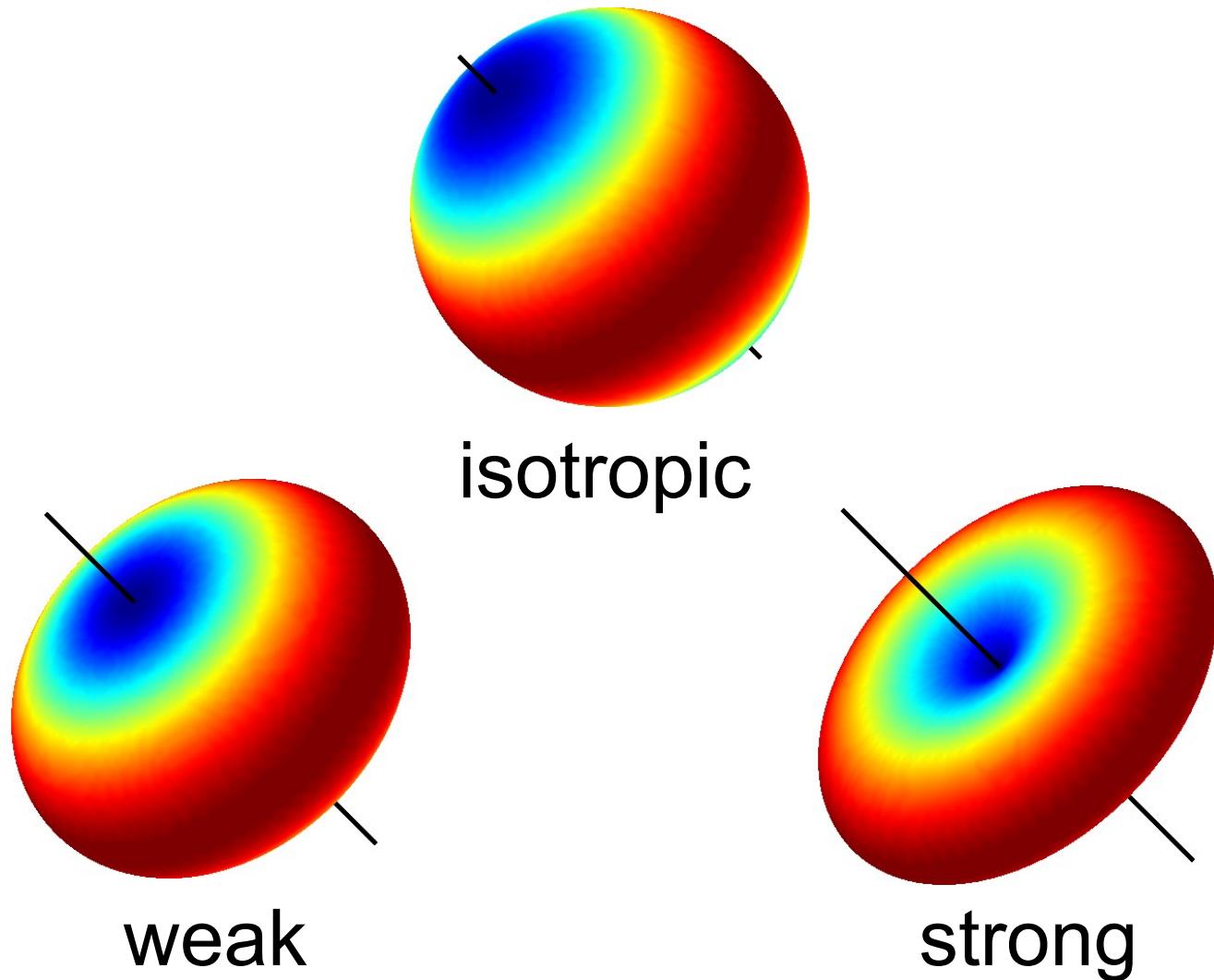
...two principal directions $\mathbf{m} \in \mathbb{R}^3$

...two scaling factors $k \in \mathbb{R}$

4 + 4 = 8 parameters

$$S(\mathbf{u}) = 0.5 e^{-k_1 (\mathbf{u}^T \mathbf{m}_1)^2} + 0.5 e^{-k_2 (\mathbf{u}^T \mathbf{m}_2)^2}$$

effect of scaling factor k



synthetic validation

brute force optimization

- matching pursuit
- parametric dictionary
- noiseless signal
- discretization, noise

spherical harmonics

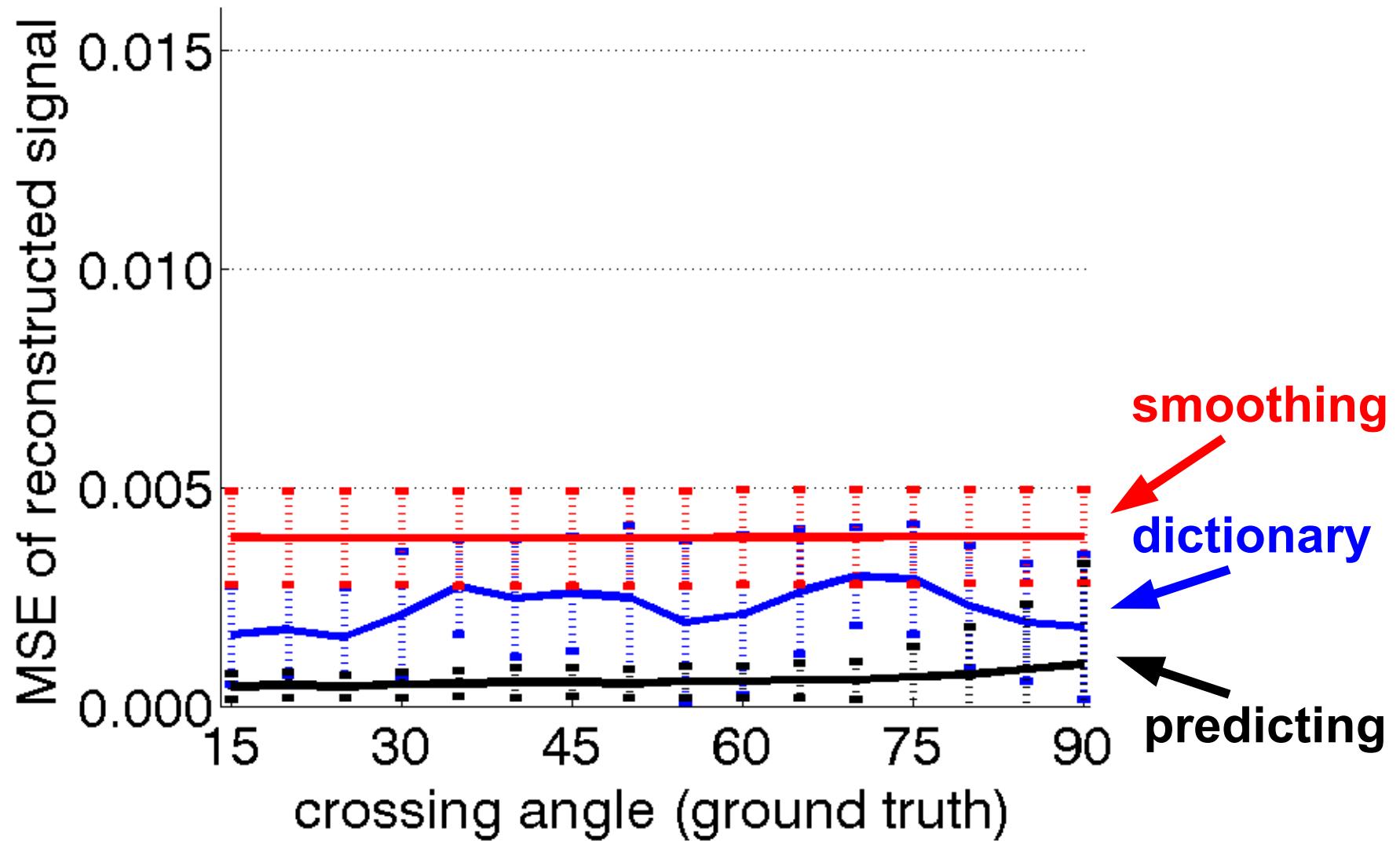
- non-parametric
- order eight (8)
- fiber sharpening for peak detection ($L=0.006$)

filtered tractography

- two-fiber model
- unscented Kalman filter

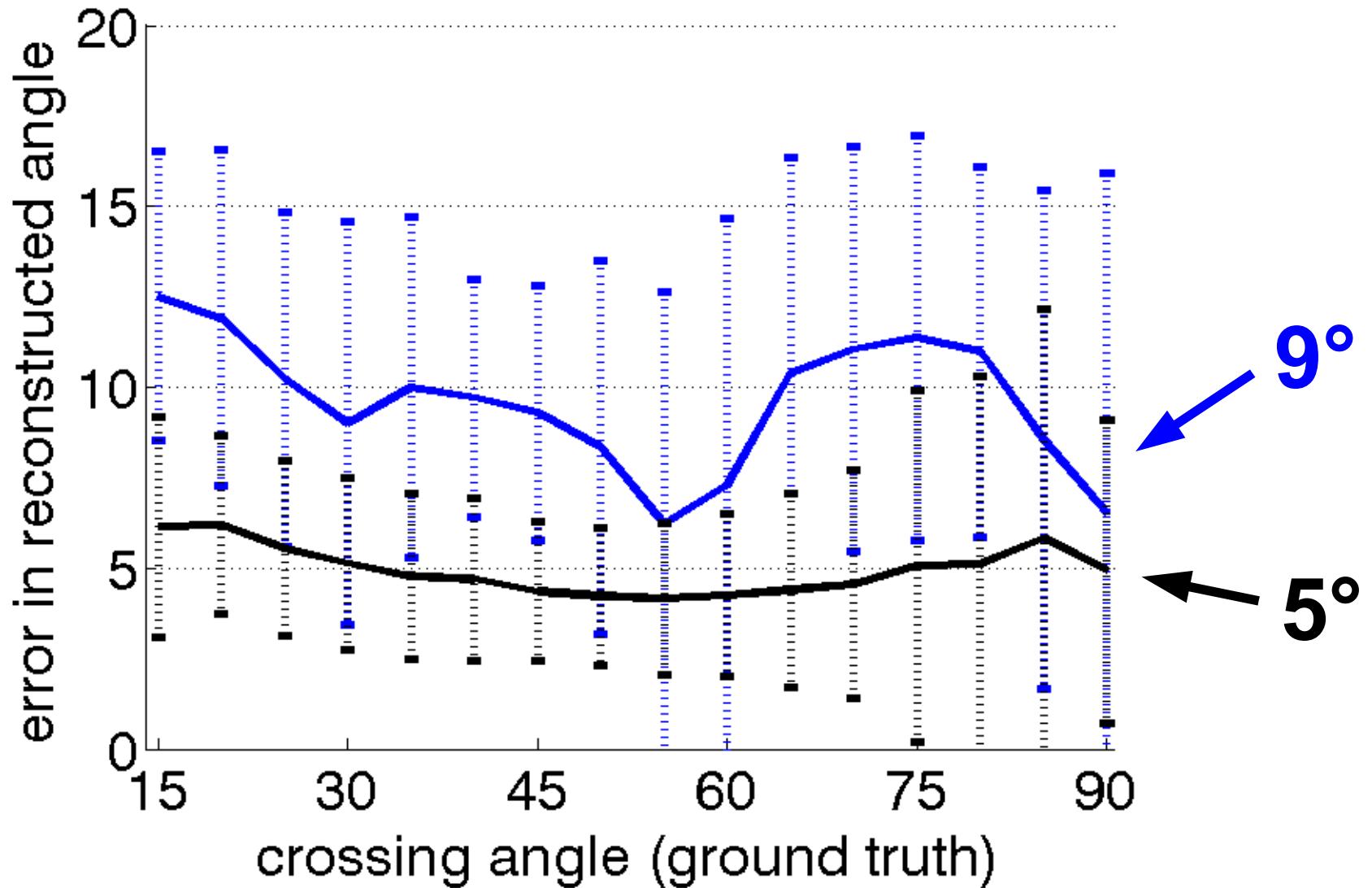
[Descoteaux 07]

signal reconstruction error



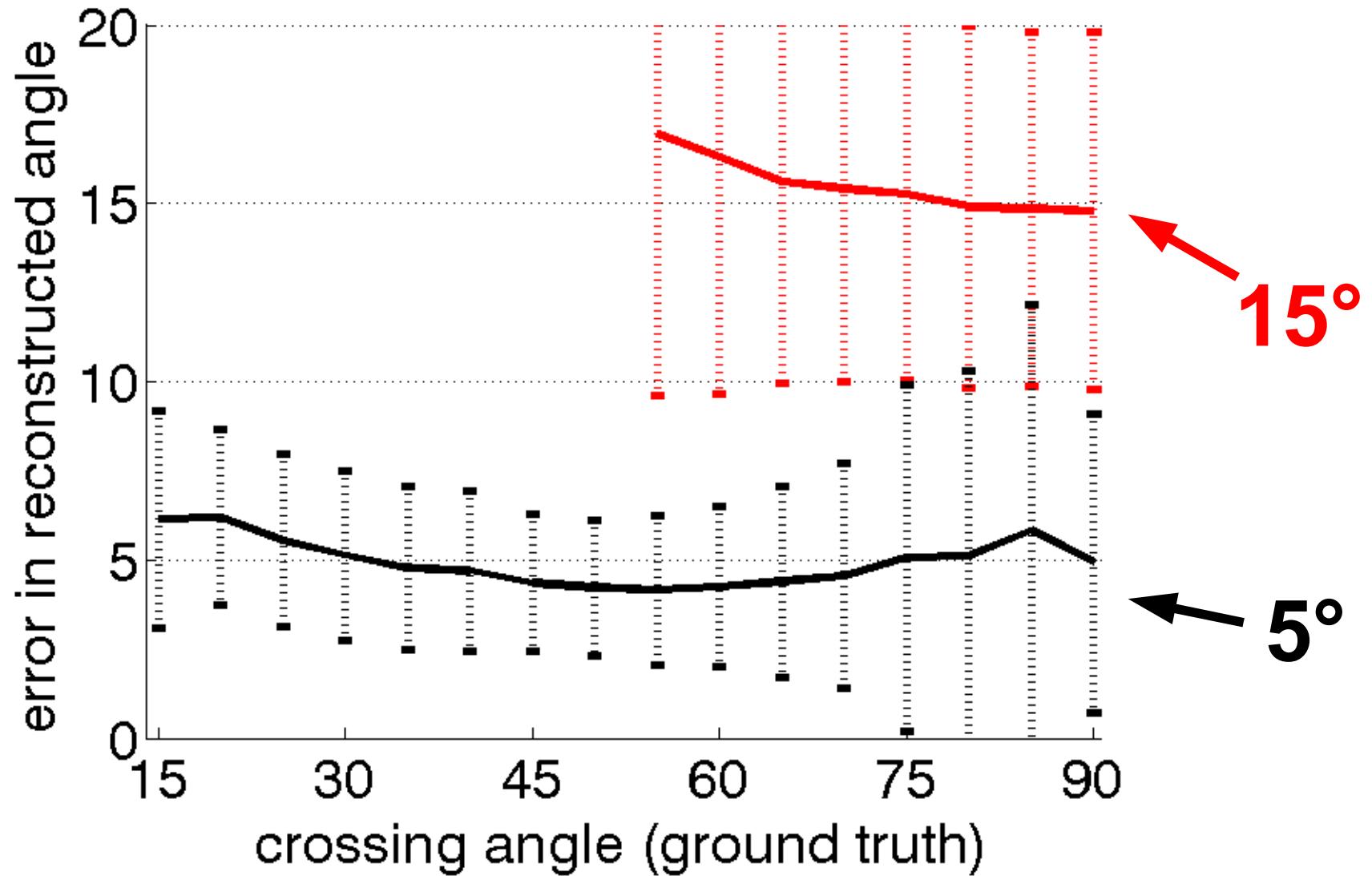
SNR ≈ 5 , b = 1000⁸⁸

angular reconstruction error



$\text{SNR} \approx 5, b = 1000^{89}$

angular reconstruction error



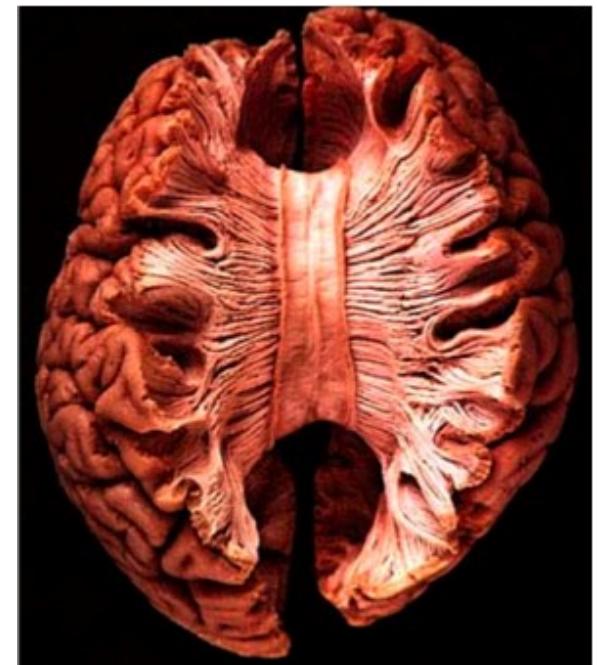
$\text{SNR} \approx 5, b = 1000^{90}$

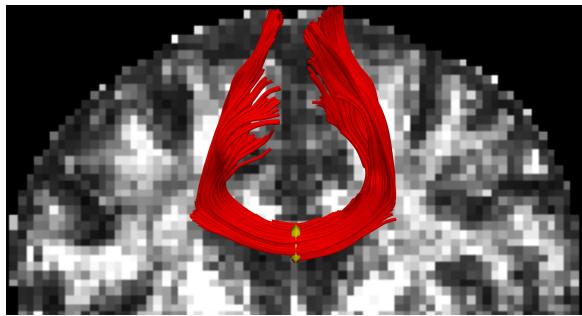


in vivo

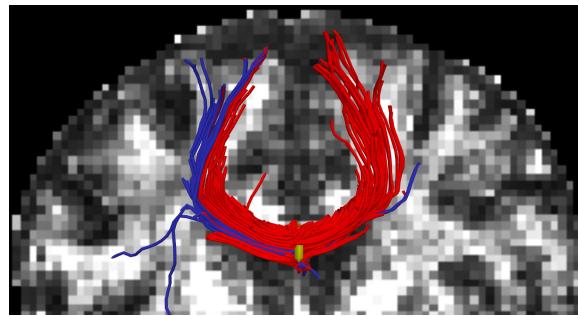


b=900
51 directions
1.7mm isotropic
voxel
17 minute scan

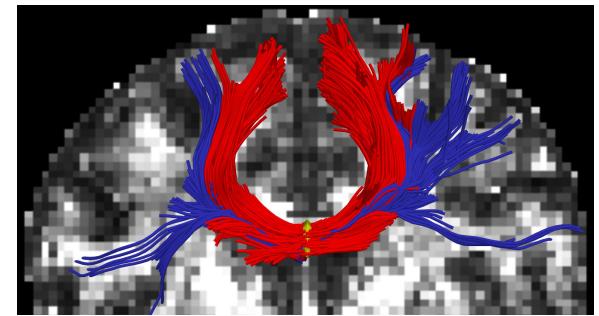




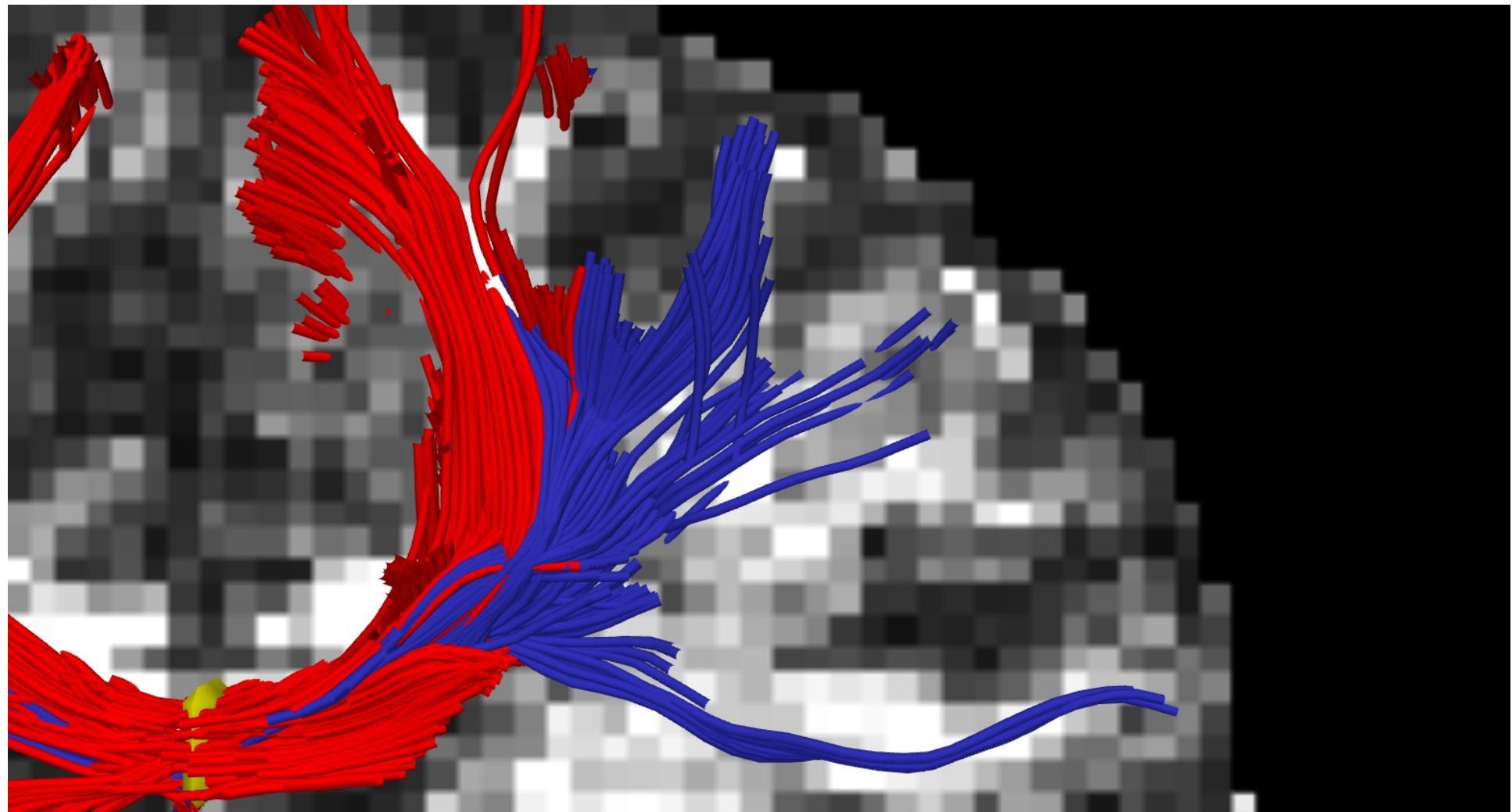
single tensor



spherical harmonics

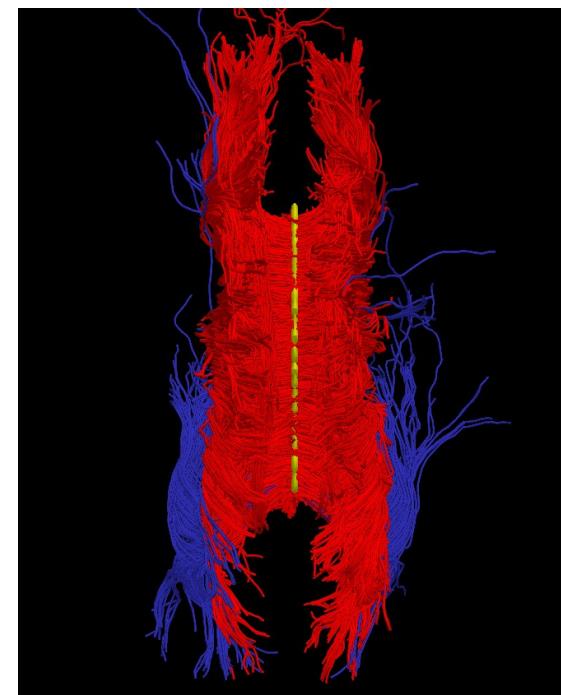
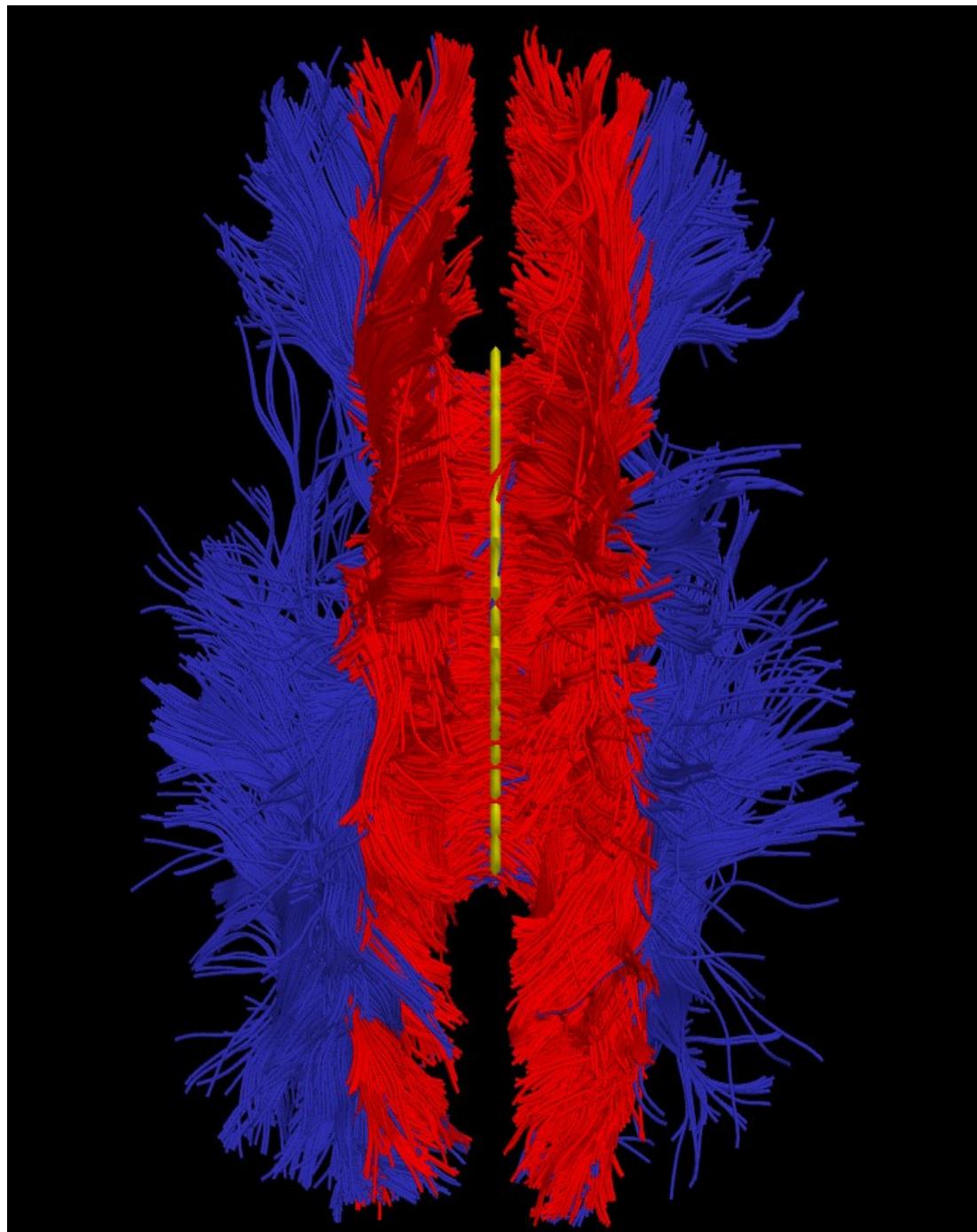


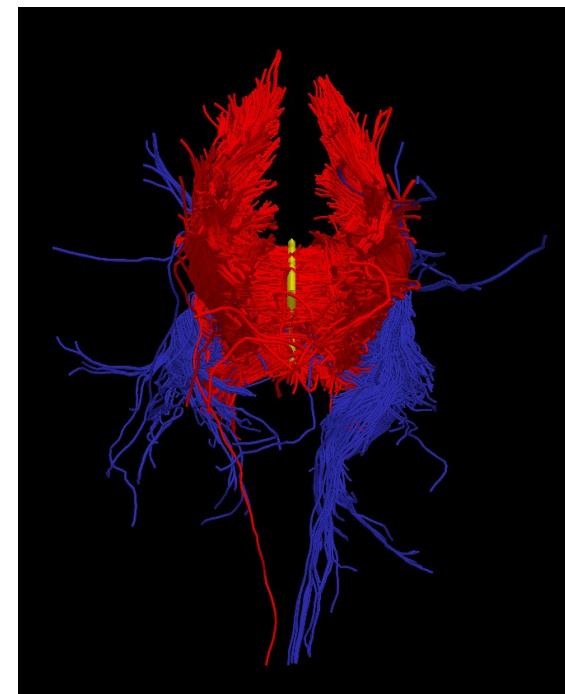
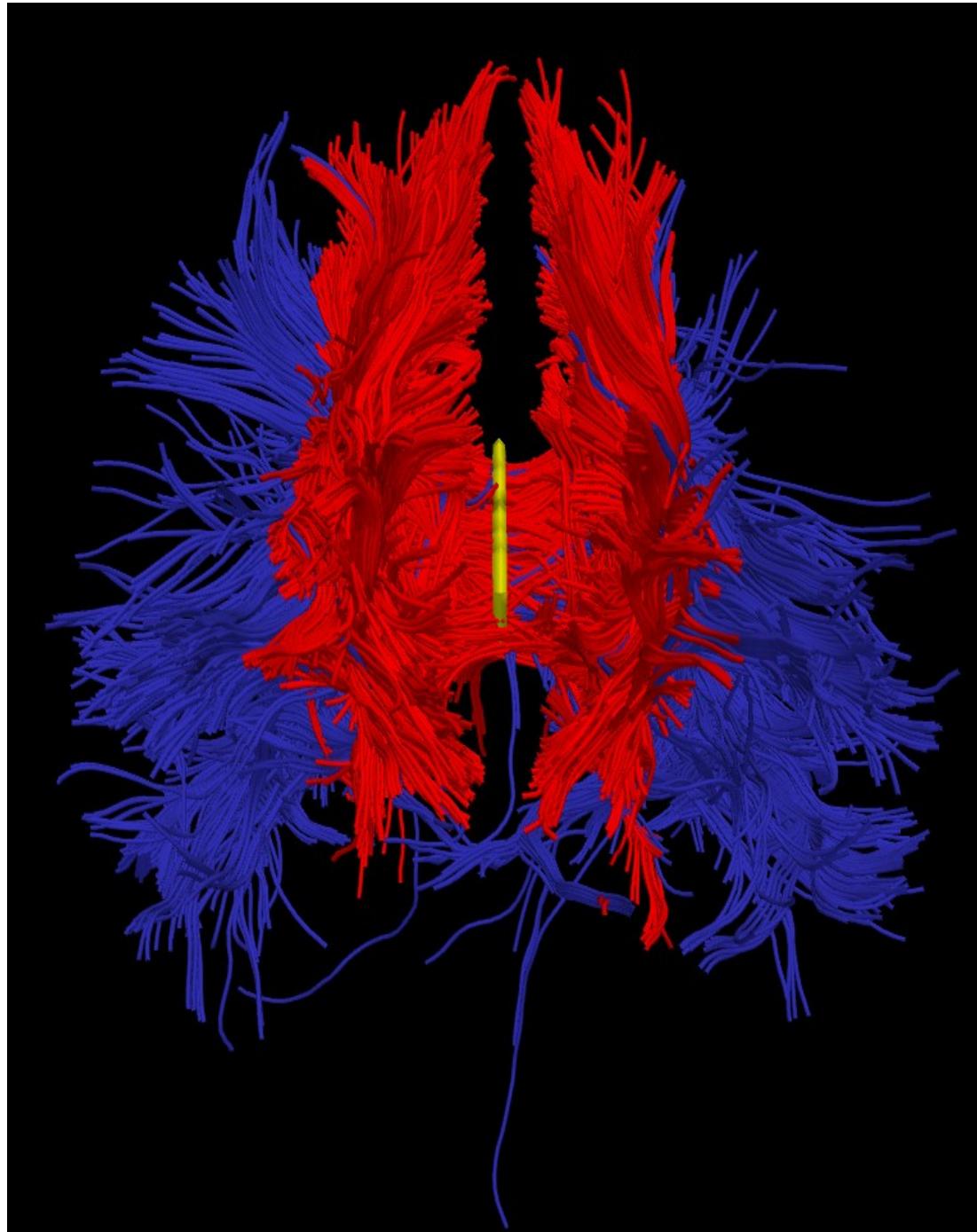
filtered two-Watson



filtered two-Watson

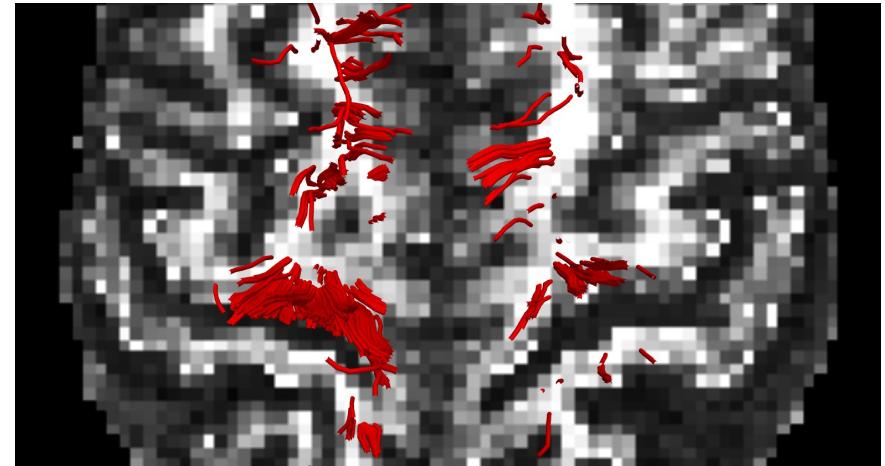
($b = 900$, 1.7mm, 51 directions)



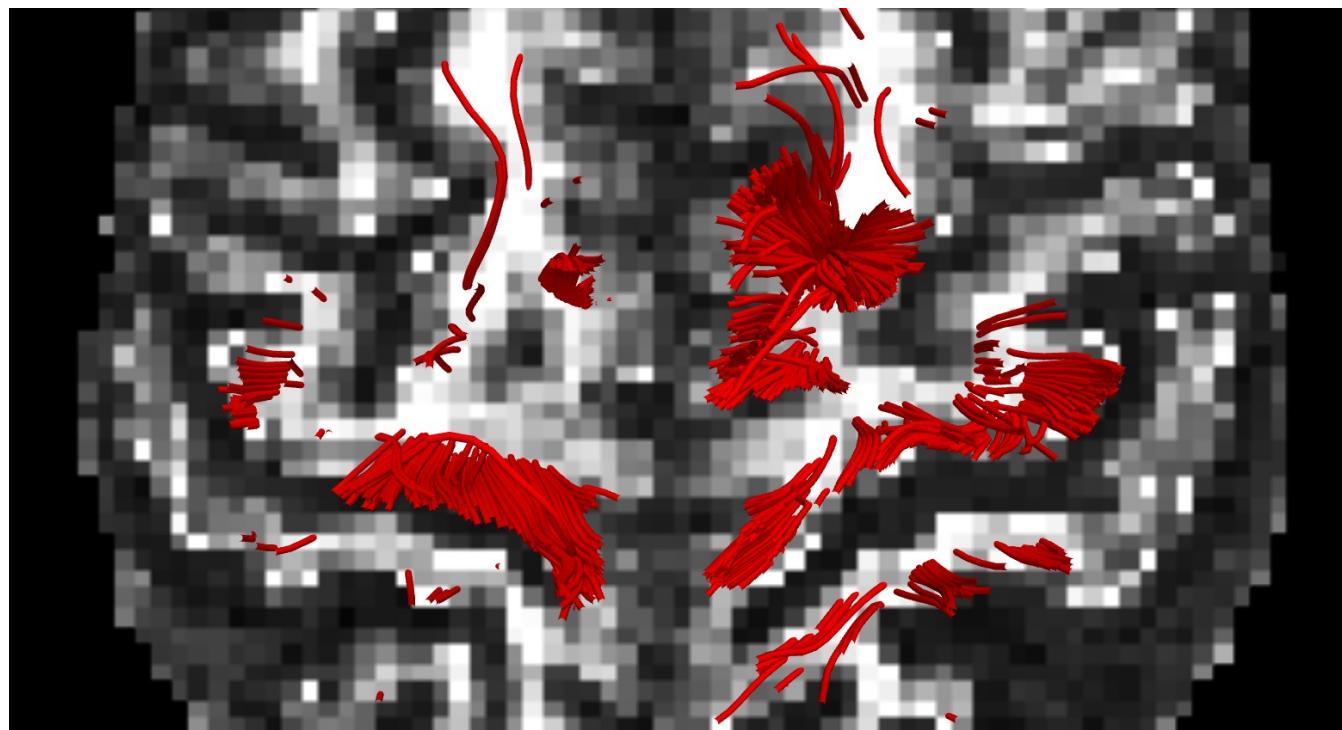




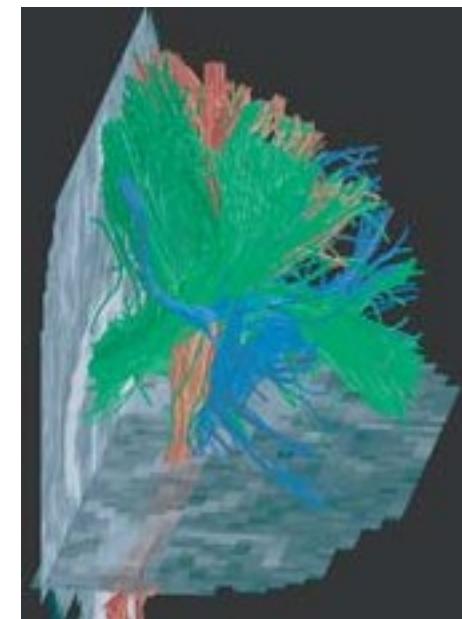
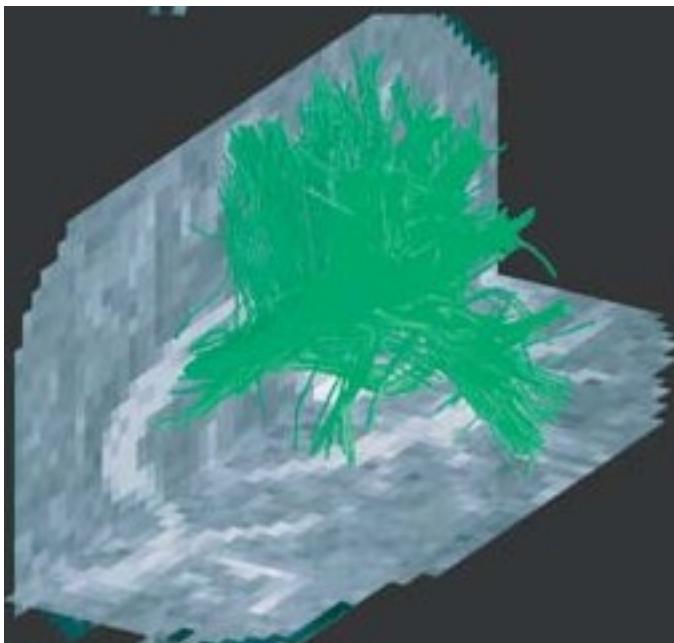
single tensor



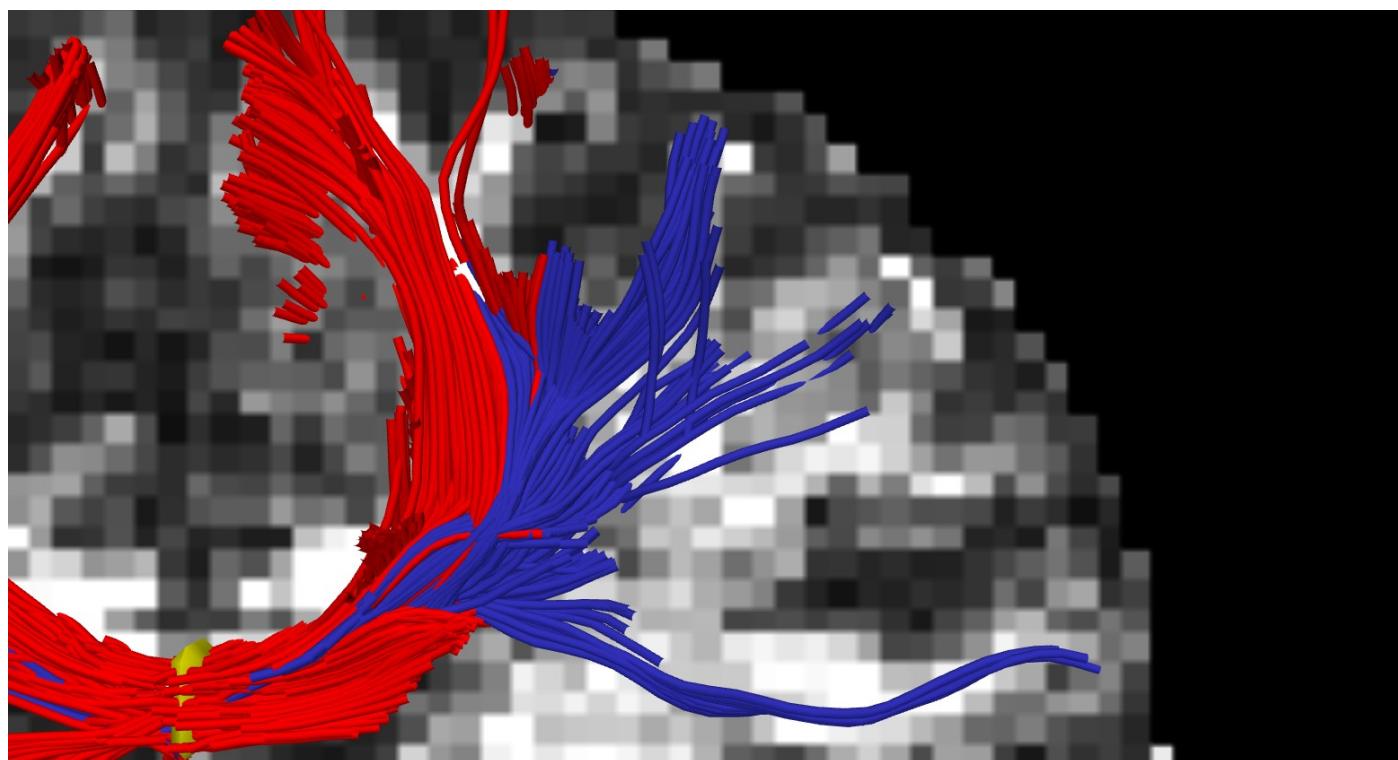
spherical harmonics



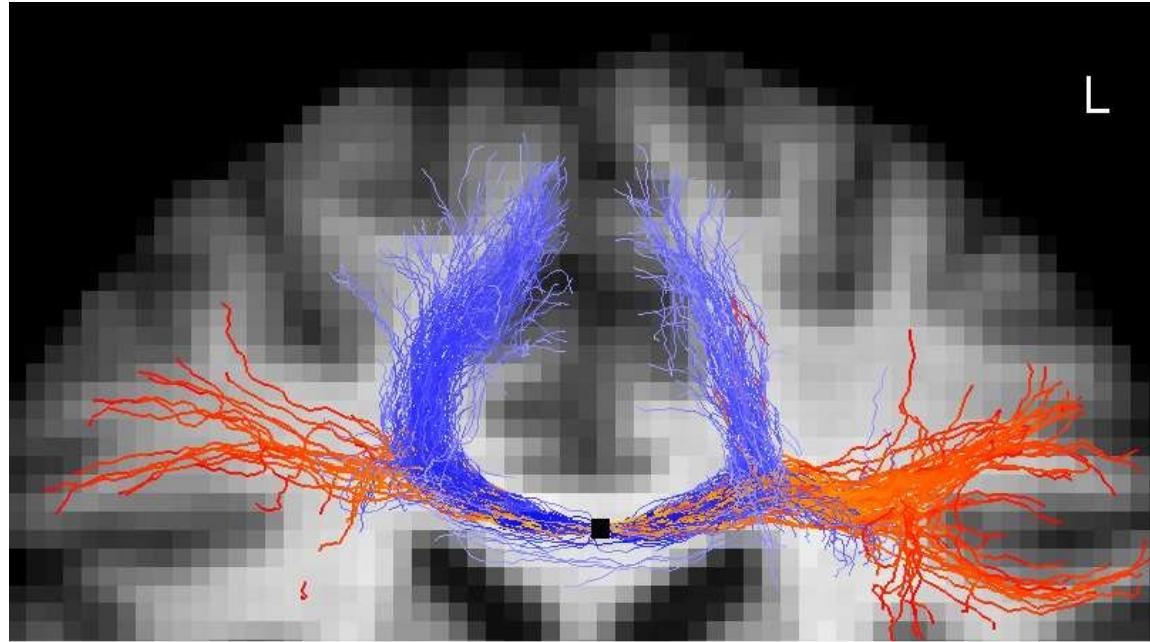
filtered two-Watson



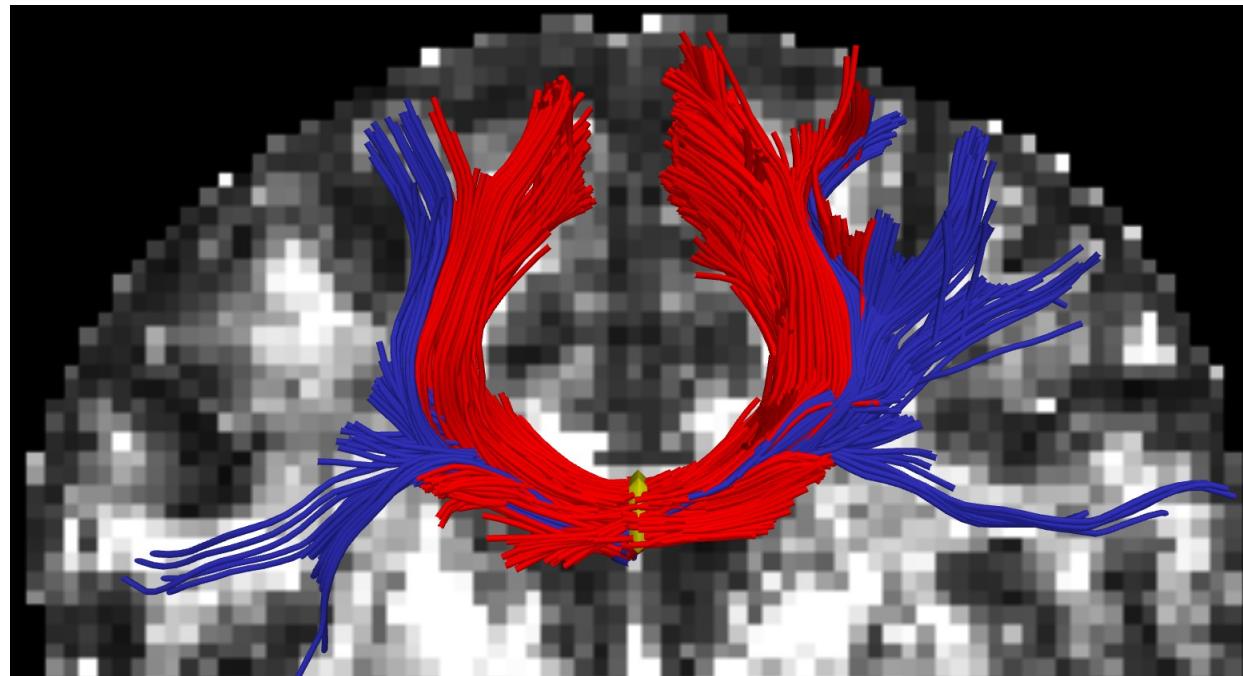
DSI [Hagmann 05]



filtered two-Watson



spherical harmonics, **probabilistic** tractography
[Descoteaux 2009]



filtered two-Watson

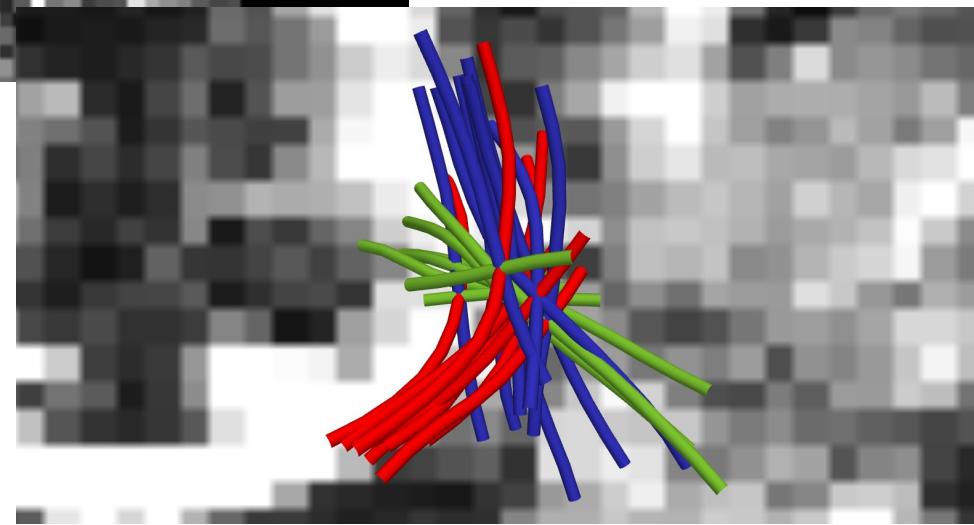
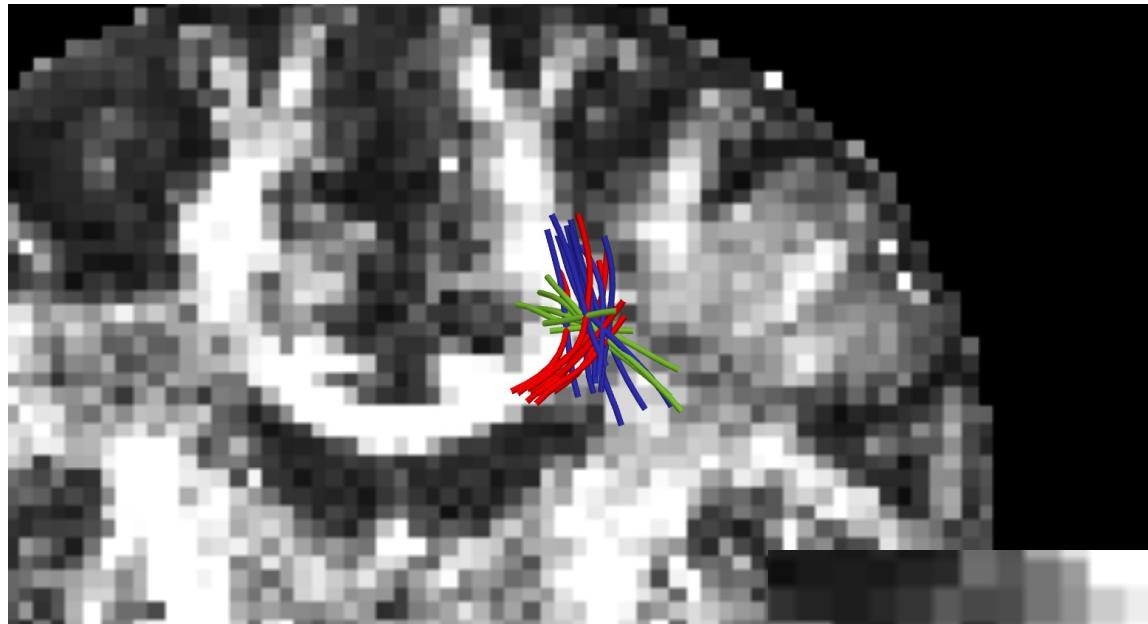
model assumptions

...in this proposal

Two fibers
single fiber: align

Fixed volume fractions
scaling factor

model selection, non-
parametric, ...



Algorithm 1 Unscented Kalman Filter

- 1: Form weighted sigma points $\mathbf{X}_t = \{w_i, \mathbf{x}_i\}_{i=0}^{2n}$ around current mean \mathbf{x}_t and covariance P_t with scaling factor ζ

$$\mathbf{x}_0 = \mathbf{x}_t \quad \mathbf{x}_i = \mathbf{x}_t + [\sqrt{\zeta P_t}]_i \quad \mathbf{x}_{i+n} = \mathbf{x}_t - [\sqrt{\zeta P_t}]_i$$

- 2: Predict the new sigma points and observations

$$\mathbf{X}_{t+1|t} = f[\mathbf{X}_t] \quad \mathbf{Y}_{t+1|t} = h[\mathbf{X}_{t+1|t}]$$

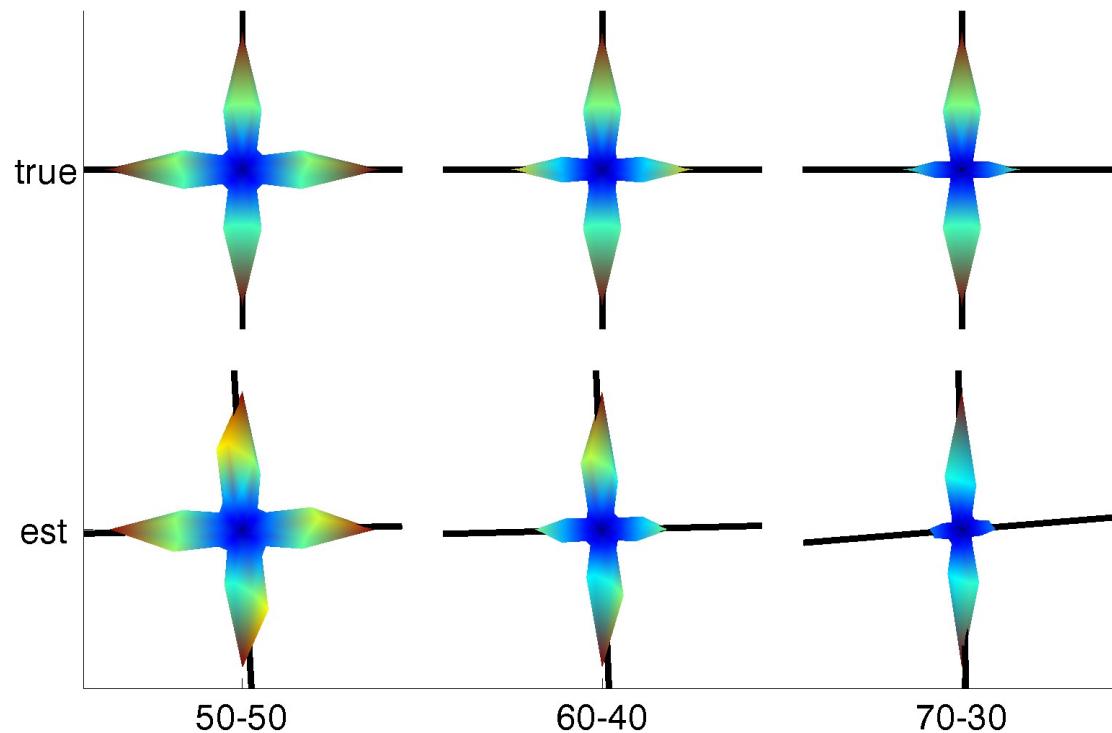
- 3: Compute weighted means and covariances, e.g.

$$\bar{\mathbf{x}}_{t+1|t} = \sum_i w_i \mathbf{x}_i \quad P_{xy} = \sum_i w_i (\mathbf{x}_i - \bar{\mathbf{x}}_{t+1|t})(\mathbf{y}_i - \bar{\mathbf{y}}_{t+1|t})^T$$

- 4: Update estimate using Kalman gain K and scanner measurement \mathbf{y}_t

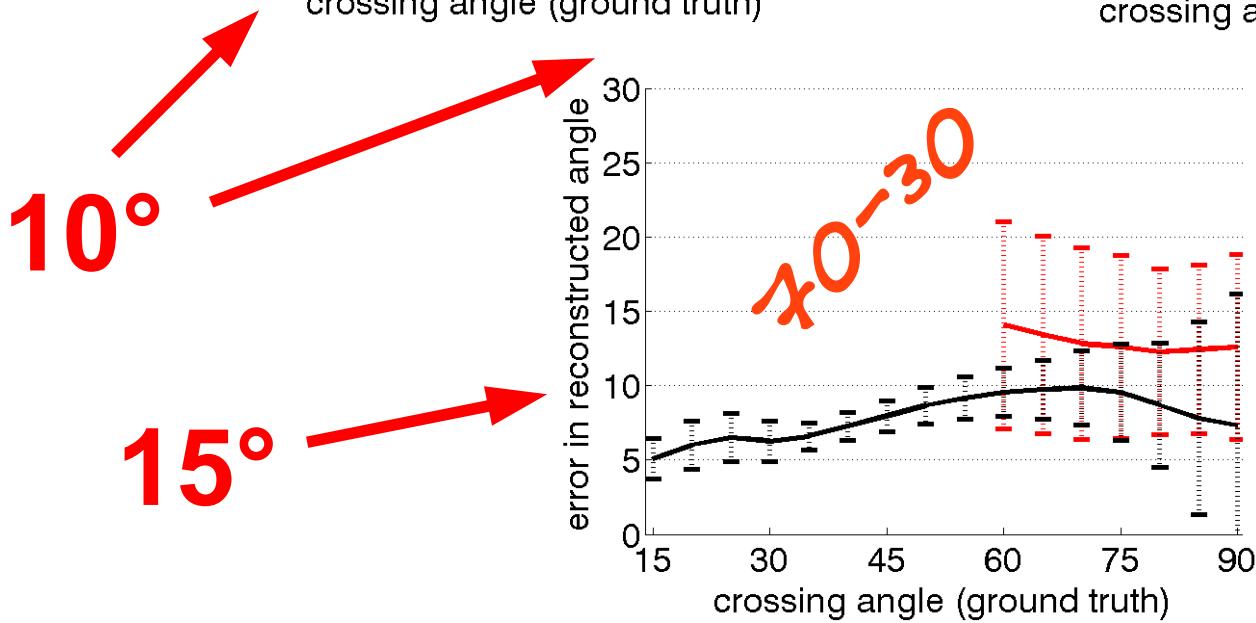
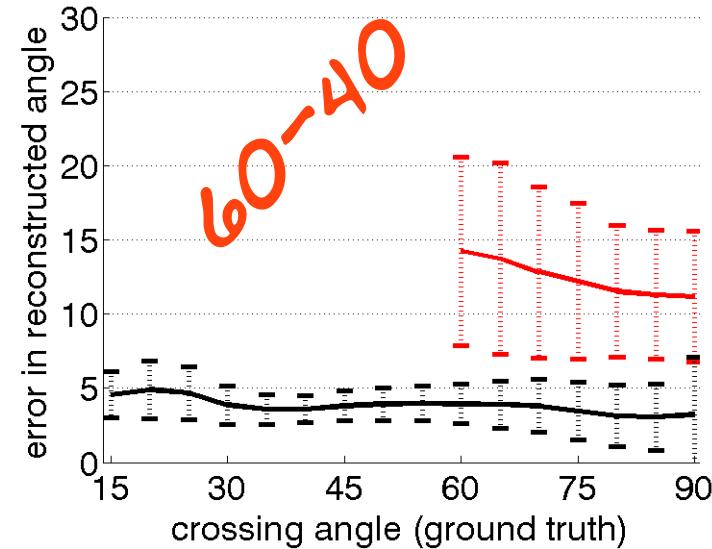
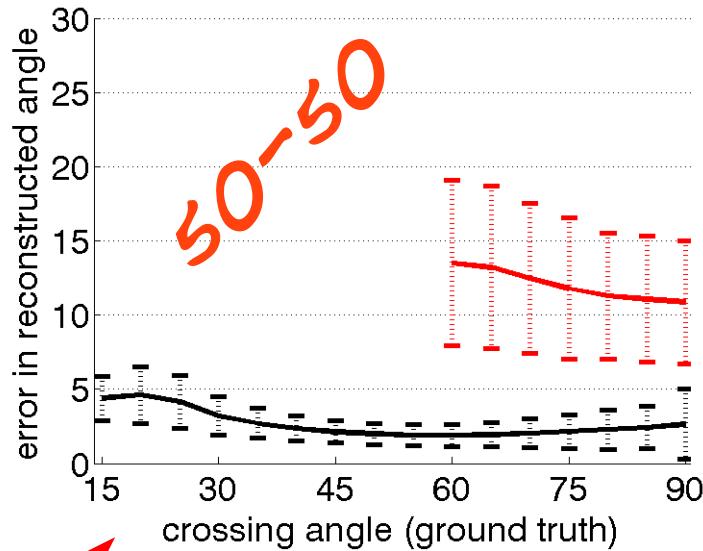
$$\mathbf{x}_{t+1} = \bar{\mathbf{x}}_{t+1|t} + K(\mathbf{y}_t - \bar{\mathbf{y}}_{t+1|t}) \quad P_{t+1} = P_{xx} - K P_{yy} K^T \quad K = P_{xy} P_{yy}^{-1}$$

volume fractions



$\text{SNR} \approx 10, b = 1000^{101}$

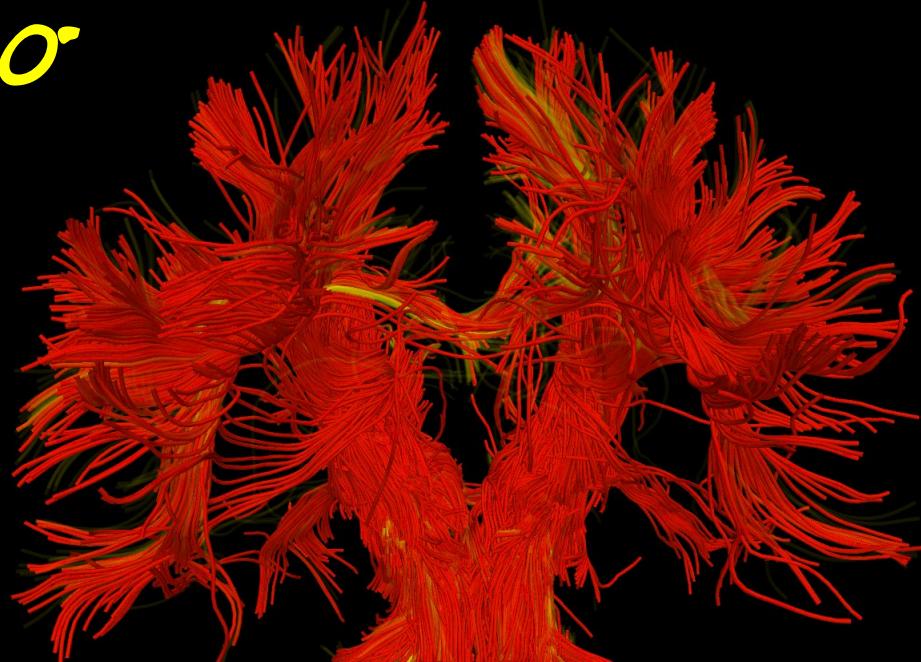
volume fractions



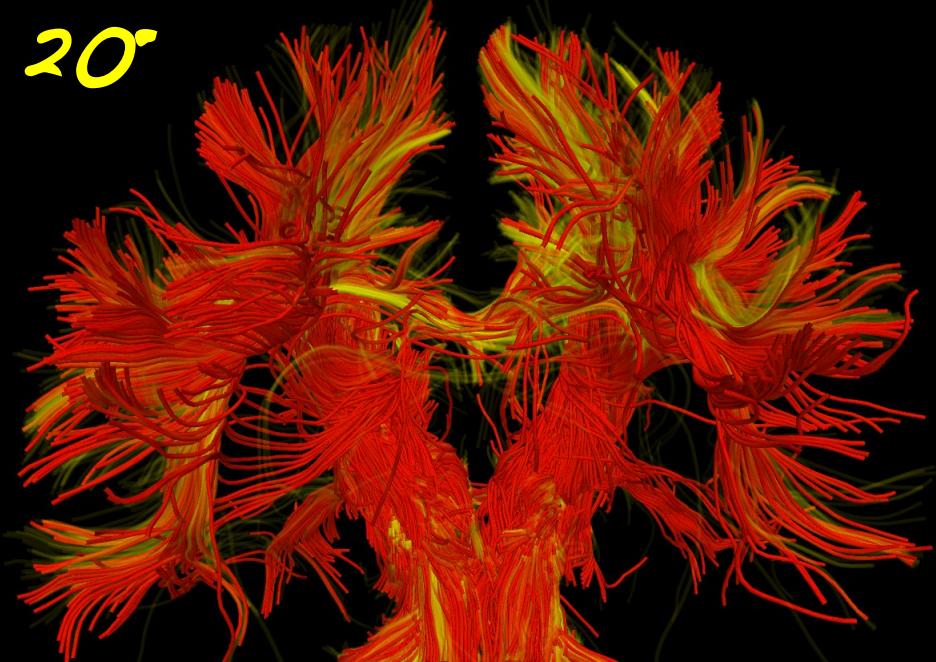
filter
deteriorates

$\text{SNR} \approx 10, b = 1000^{102}$

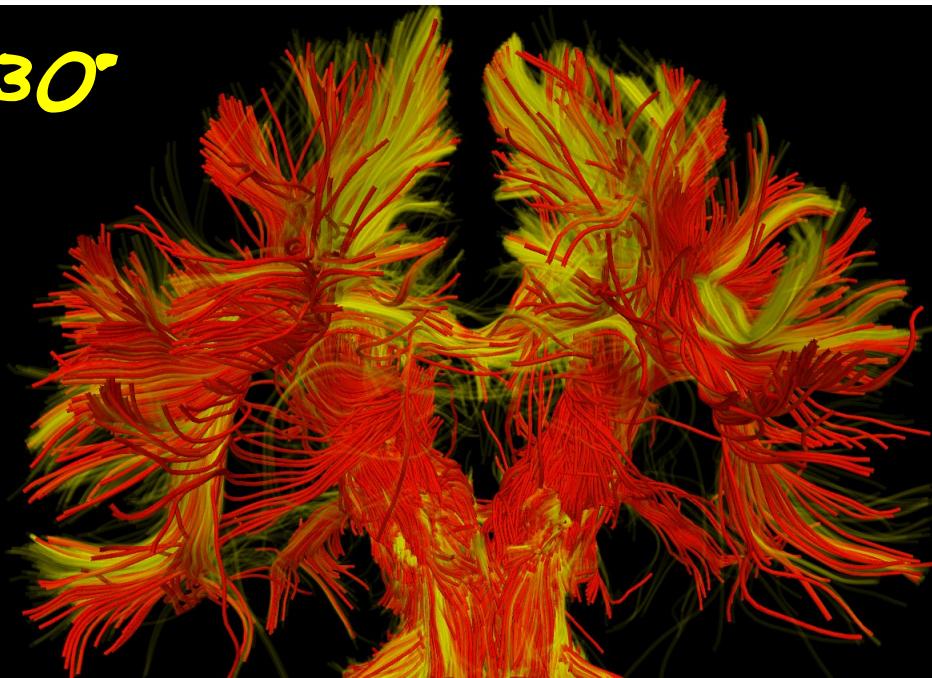
10°



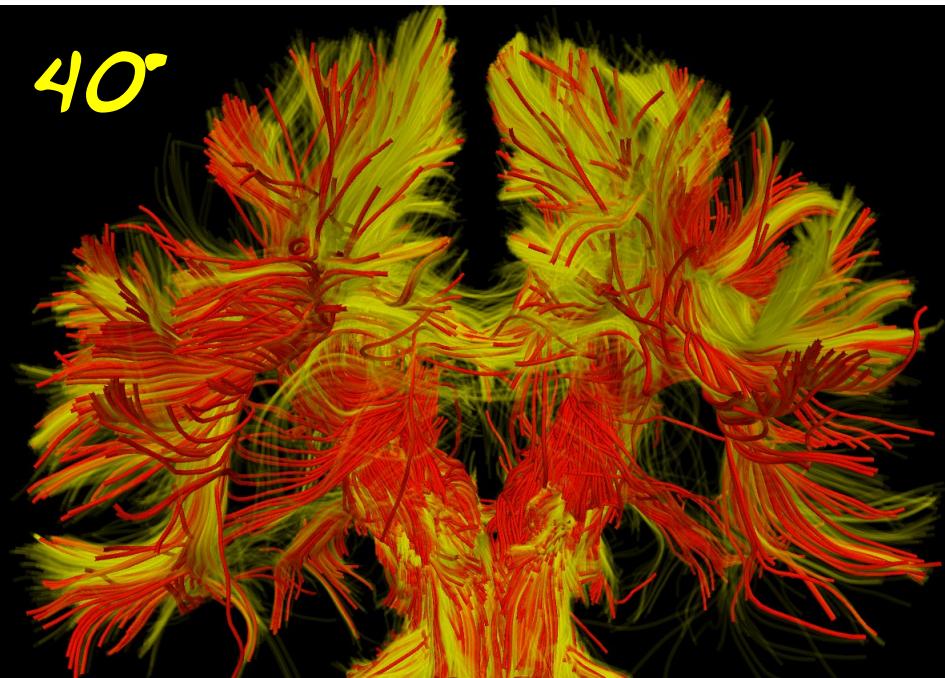
20°



30°

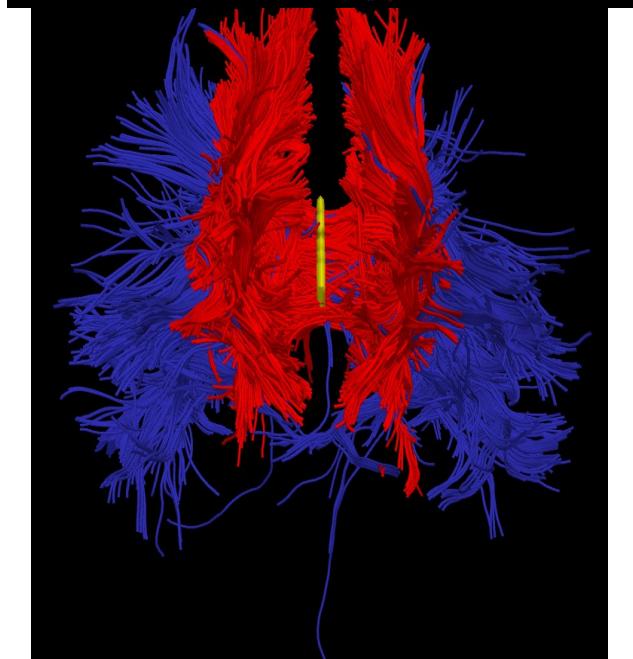
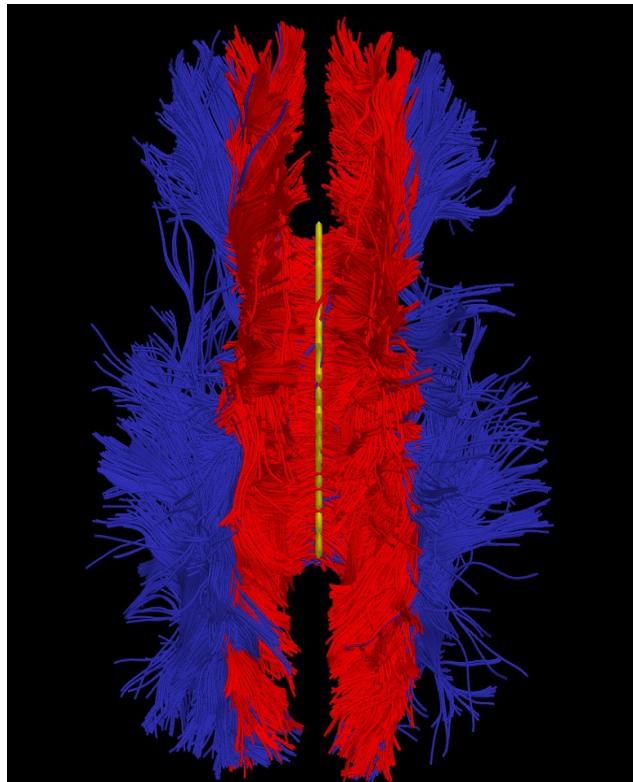


40°



primary

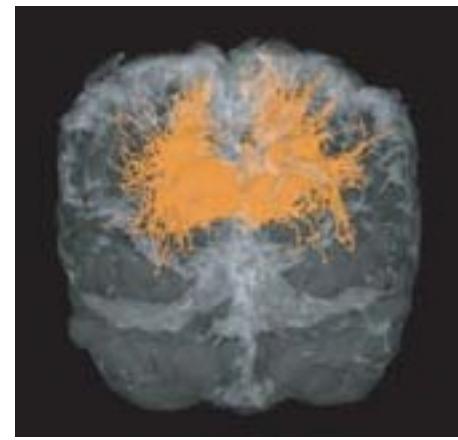
branches



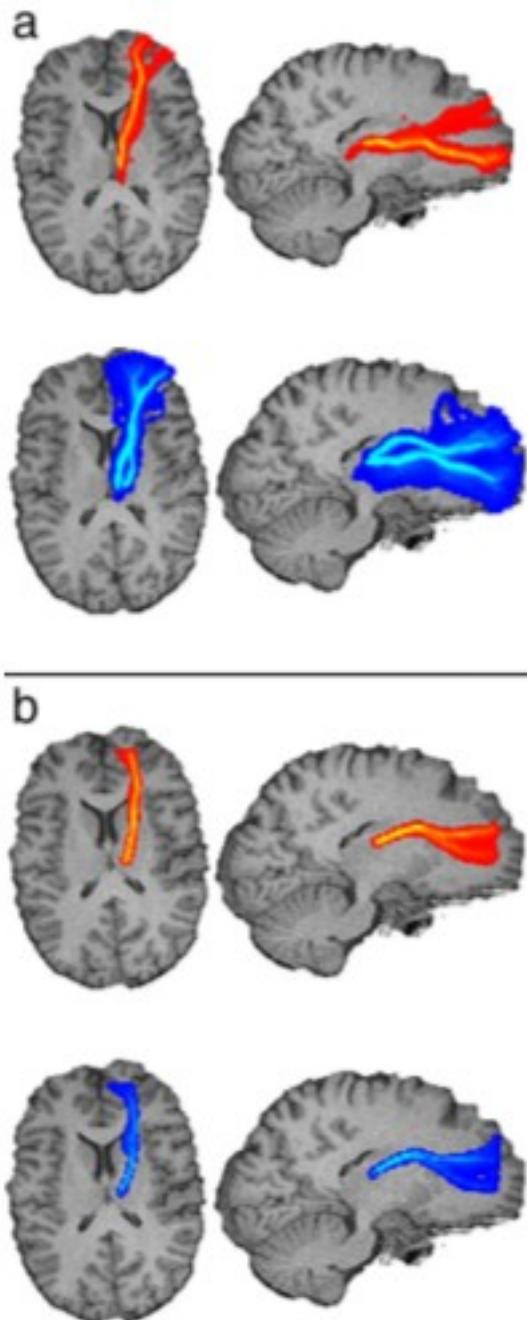
filtered two-Watson



DSI (Hagmann 2005)

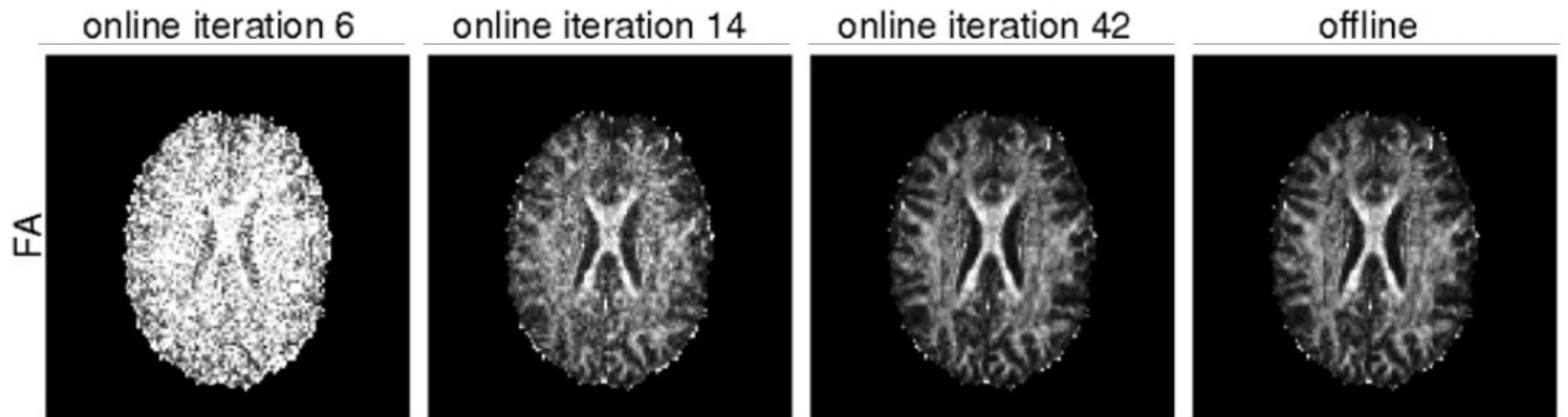


DSI (Hagmann 2005)

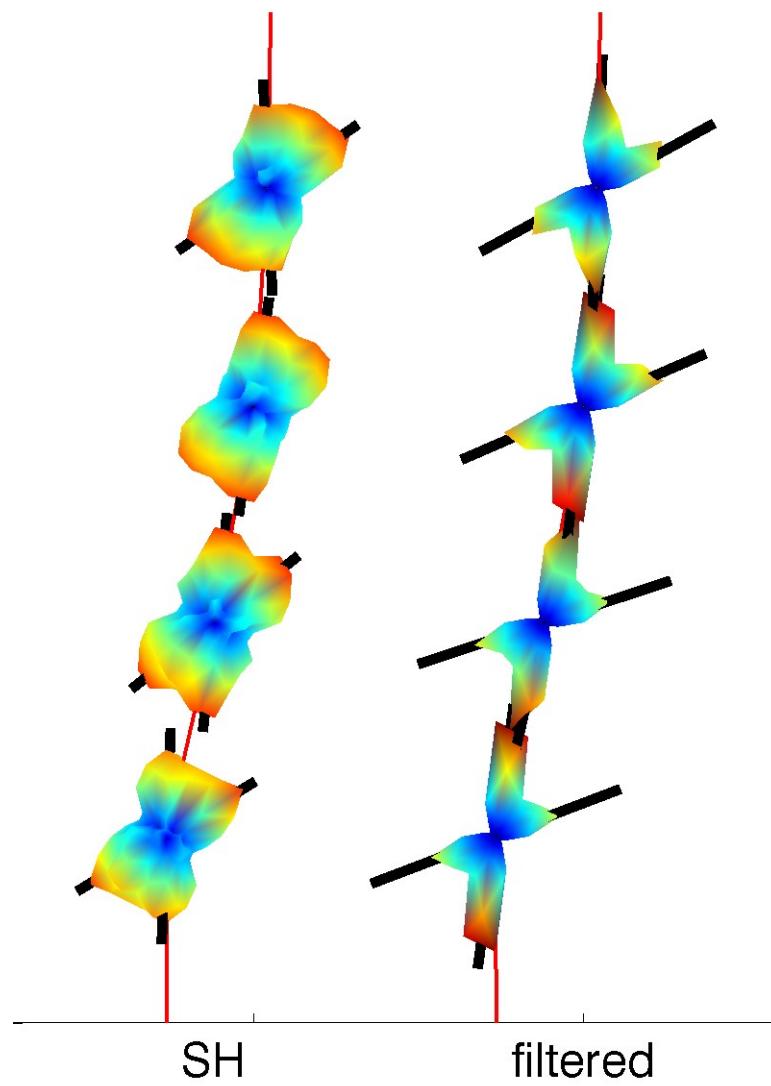
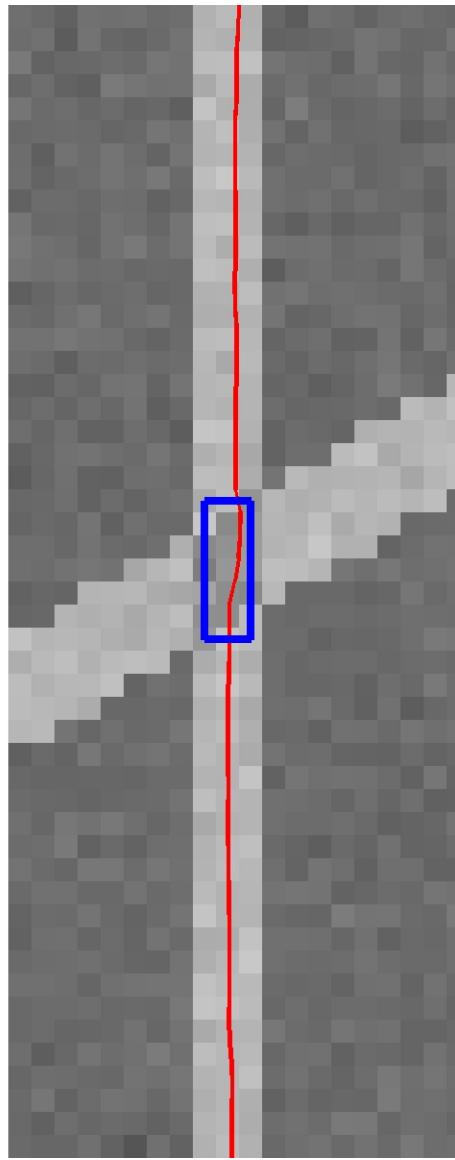


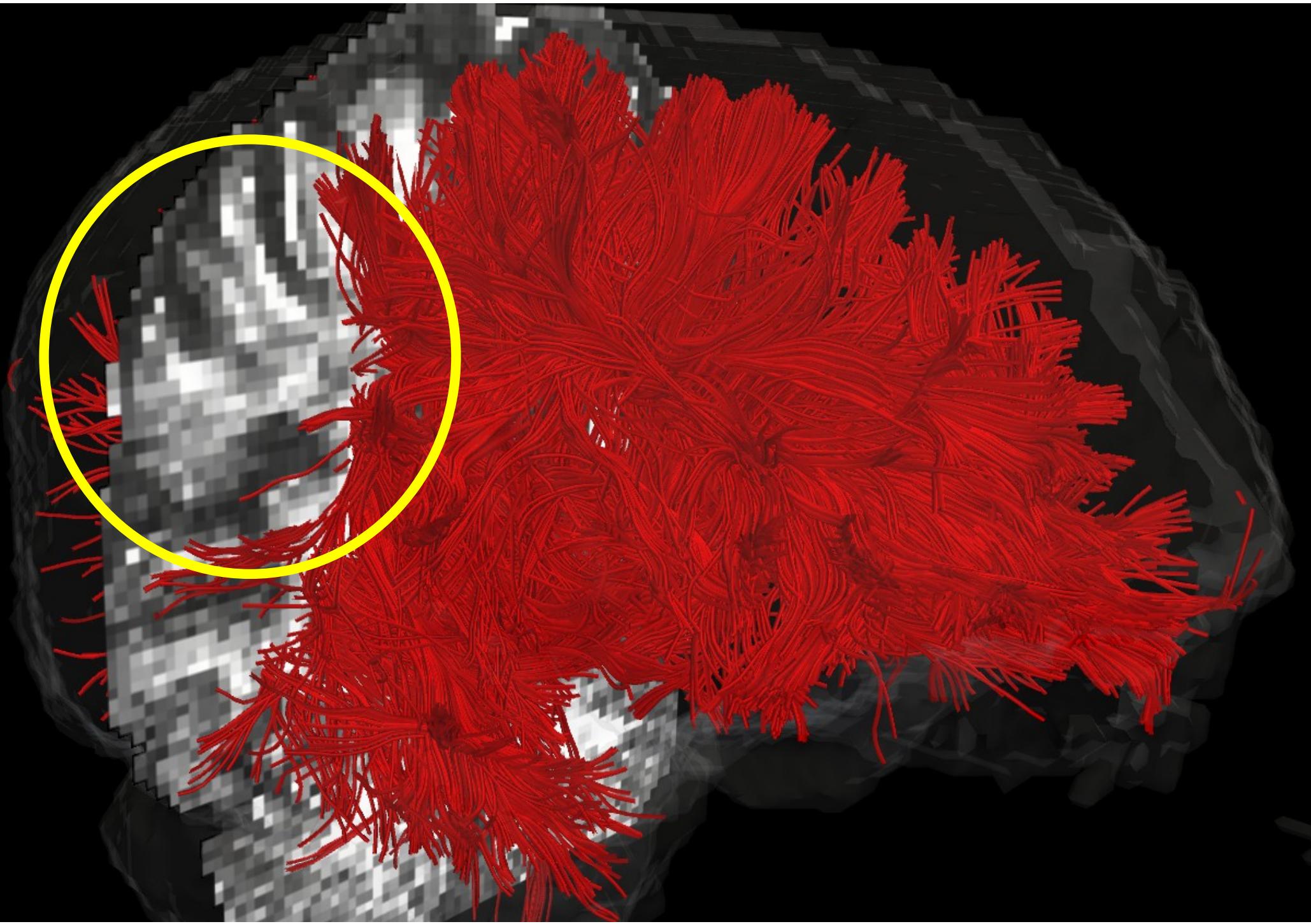
[Jababdi 07]

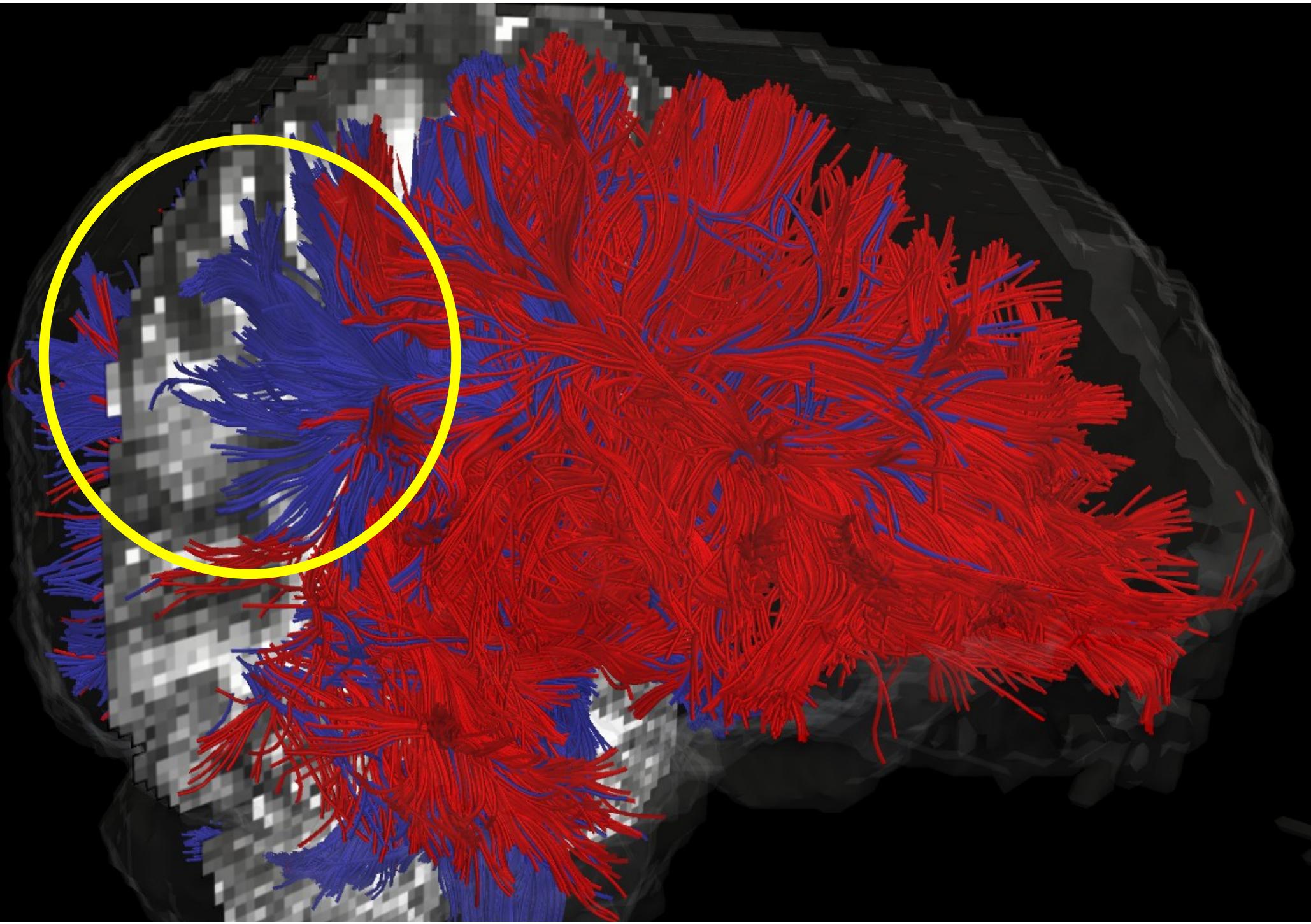
ROI-based
to constrain
probabilistic

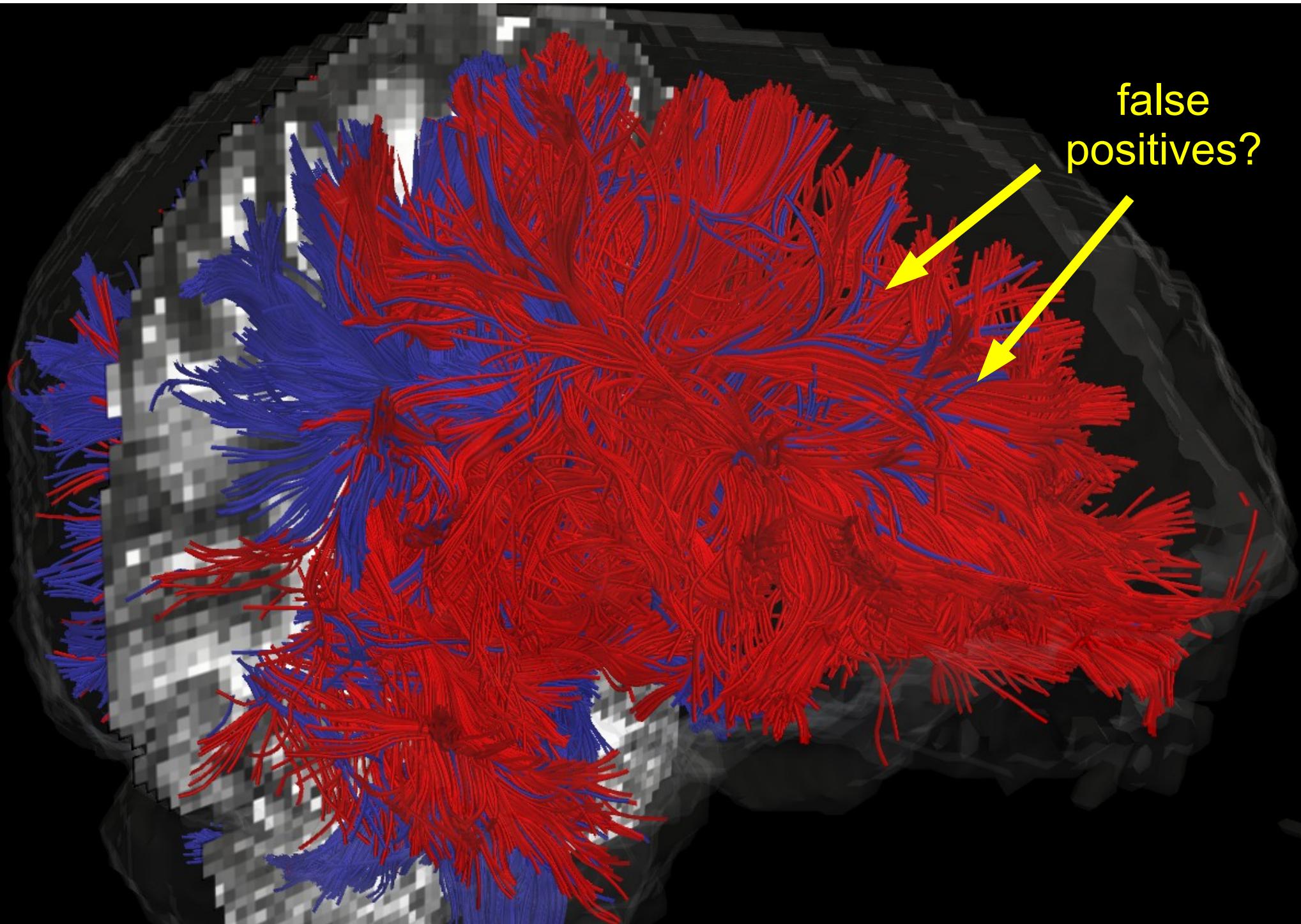


[Poupon 08, Deriche 09]



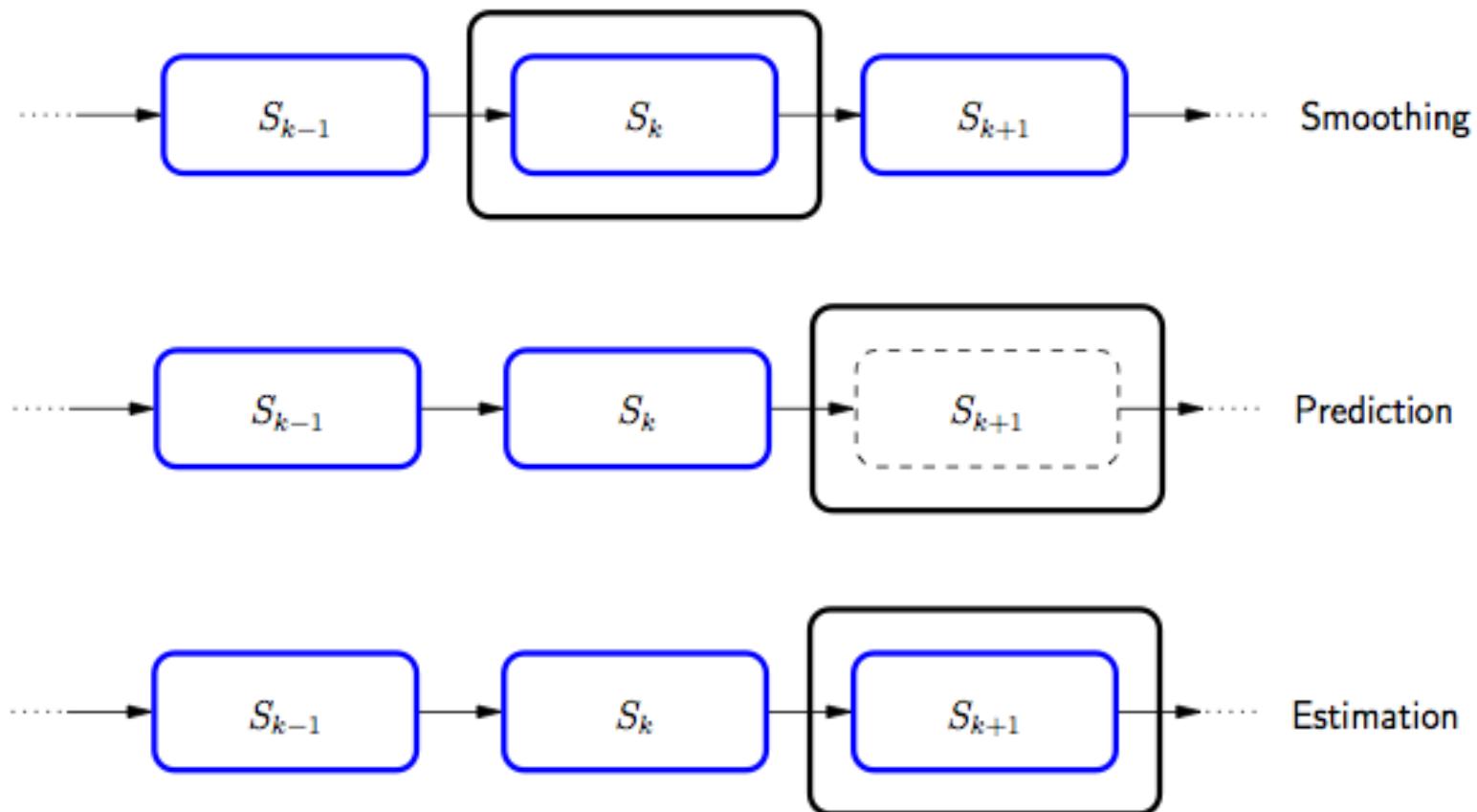






false
positives?

filtering



[Niethammer 08]

brute force optimization

- matching pursuit
- parametric dictionary
- noiseless signal
- discretization, noise

spherical harmonics

- non-parametric
- order eight (8)
- fiber sharpening for peak detection ($L=0.006$)

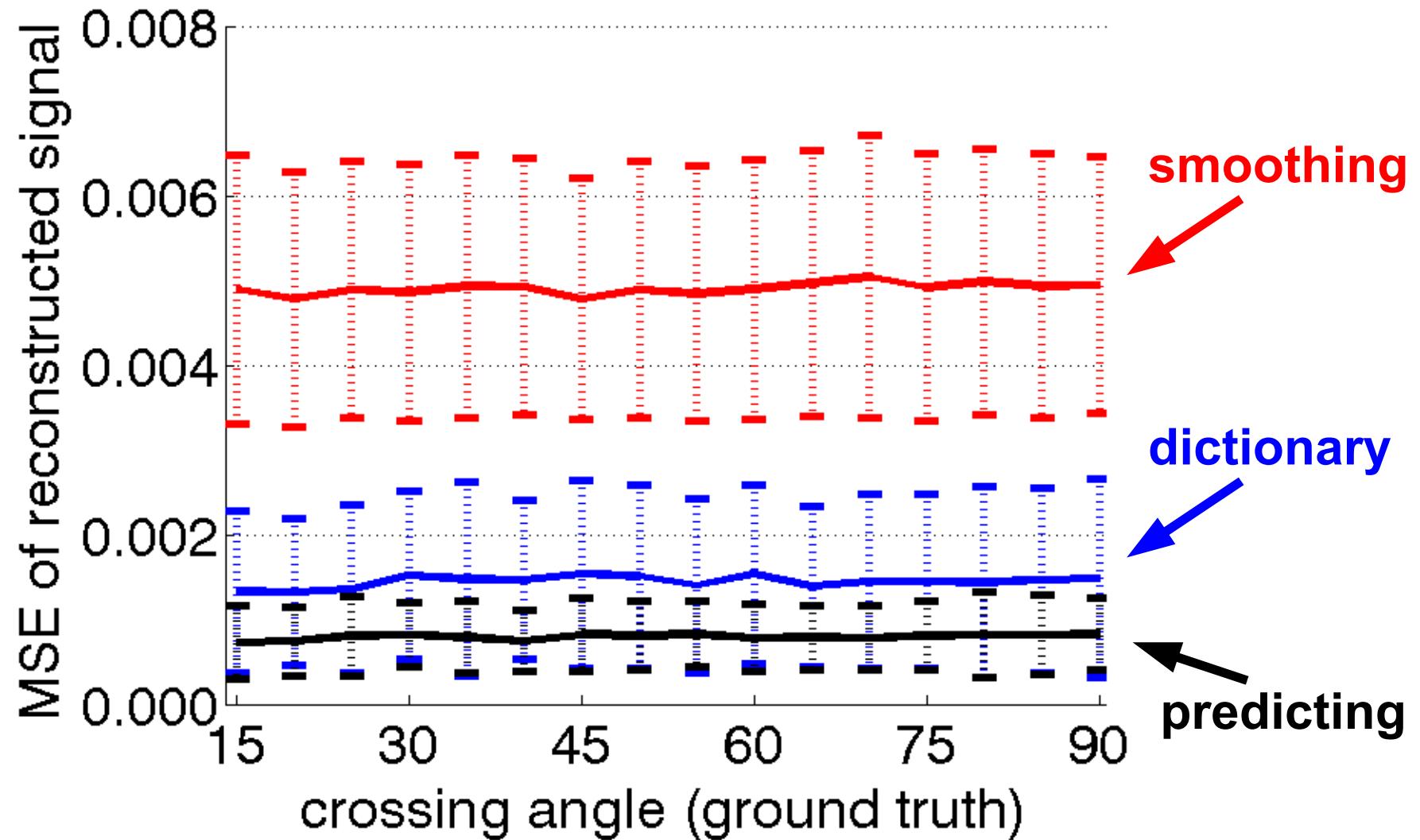
filtered tractography

- two-fiber model
- unscented Kalman filter

[Descoteaux 07]

J. G. Malcolm, M. E. Shenton, and Y. Rathi. Neural tractography using an unscented Kalman filter. In *Information Processing in Medical Imaging (IPMI)*, pages 126–138, 2009.

signal reconstruction error



SNR ≈ 5 , b = 1000