

ANALYSIS OF LOCAL IMAGE STATISTICS TO IMPROVE MEDICAL IMAGE PROCESSING

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**PROPOSAL EXAM
MARCH 3, 2009**

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OUTLINE

- Quick Background
- Localized Approach
- Preliminary Research
- Proposed Research

BACKGROUND

COMPUTER VISION

- Acquisition and Filtering
- Segmentation, Tracking, and Analysis
- Interpretation and Assigning Meaning

SEGMENTATION



SEGMENTATION

- Thresholding
- Region Growing
- Graph Cuts
- Snakes / Active Contours

ACTIVE CONTOURS



IMPLEMENTATION

- Represent the contour
- Parametrized
- Non-parametrized

LEVEL SETS



DEFINITIONS

- Image, $I: \mathbb{R}^n \rightarrow \mathbb{R}$ on the domain Ω
- Contour, C embedded in $\phi: \mathbb{R}^n \rightarrow \mathbb{R}$
- Such that: $C = \{x | \phi(x) = 0\}$

Sethian. Level Set Methods and Fast Marching Methods. 1999

DEFINITIONS

$$\mathcal{H}\phi = \begin{cases} 1 & \phi < -\epsilon \\ 0 & \phi > \epsilon \\ \text{smooth} & \text{otherwise} \end{cases}$$

$$\delta\phi = \begin{cases} 1 & \phi = 0 \\ 0 & |\phi| < \epsilon \\ \text{smooth} & \text{otherwise} \end{cases}$$

DEFINE AN ENERGY

- Make an assumption
- Craft an energy accordingly

Mumford and Shah “Boundary Detection by Minimizing Functionals,” JIU, 1988

UNIFORM MEAN ENERGY

Assumption: The foreground and background will be approximately constant.

$$\begin{aligned} E(\phi) = & \int_{\Omega} \mathcal{H}\phi(I - \mu_{\text{in}})^2 \\ & + (1 - \mathcal{H}\phi)(I - \mu_{\text{out}})^2 dx \\ & + \lambda \int_{\Omega} \delta\phi(x) \|\nabla\phi(x)\| dx \end{aligned}$$

Chan and Vese. “Active contours without edges,” TIP, 2001

ENERGY MINIMIZATION

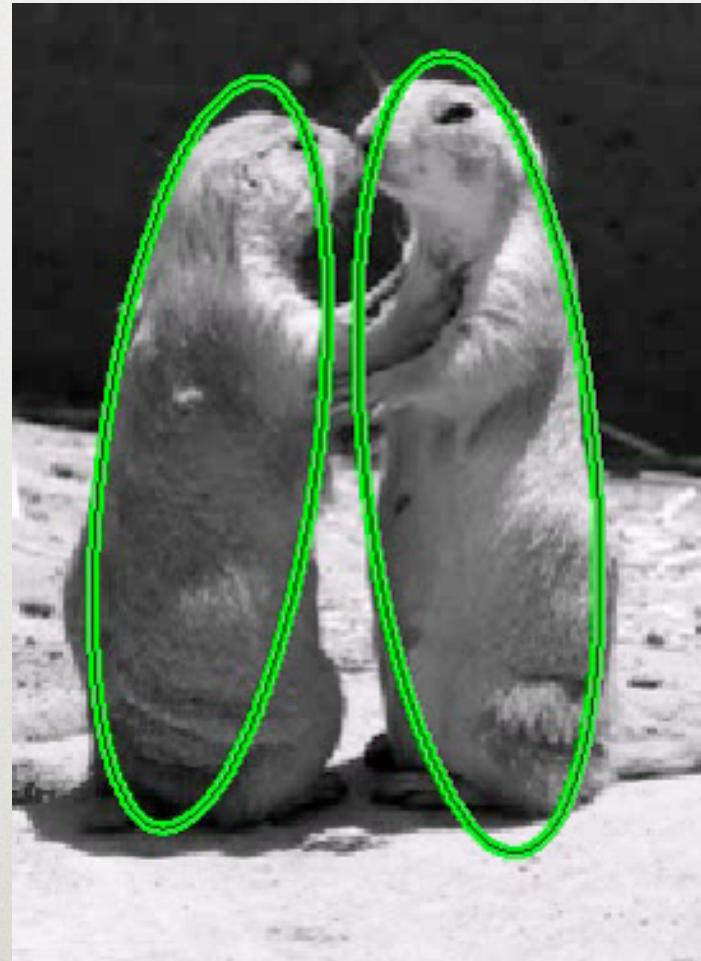
$$\frac{d\phi}{dt} = -\delta\phi \left((I - \mu_{\text{in}})^2 - (I - \mu_{\text{out}})^2 + \lambda \operatorname{div} \left(\frac{\nabla\phi}{|\nabla\phi|} \right) \right)$$

$$\phi_{t+1} = \phi_t + dt \cdot \frac{d\phi}{dt}$$

ENERGY MINIMIZATION

- Global minima
- Almost-global minima
- Local minima

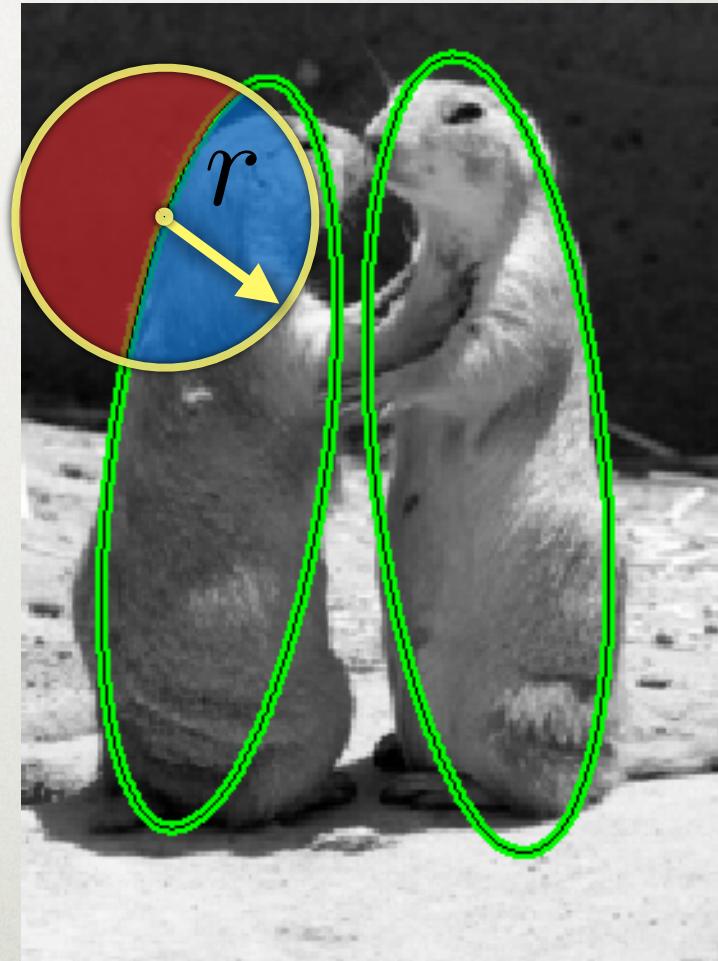
THINGS GET HARDER



LOCALIZED APPROACH

LOCALIZING

$$\begin{aligned} & x \\ & \mathcal{B}(x, y) \\ & \mathcal{B}(x, y) \cdot \mathcal{H}\phi(y) \\ & \mathcal{B}(x, y) \cdot (1 - \mathcal{H}\phi(y)) \end{aligned}$$



Lankton and Tannenbaum "Localized Region-Based Active Contours," TIP, 2008

LOCALIZED CONTOURS

$$E(\phi) = \int_{\Omega_x} \delta\phi(x) \int_{\Omega_y} \mathcal{B}(x, y) \cdot F(I(y), \phi(y)) dy \ dx$$

$$+ \lambda \int_{\Omega_x} \delta\phi(x) \|\nabla\phi(x)\| dx$$

$$\frac{\partial \phi}{\partial t}(x) = -\delta\phi(x) \int_{\Omega_u} \mathcal{B}(x, y) \cdot \nabla_{\phi(y)} F(I(y), \phi(y)) dy + \lambda \delta\phi(x) \operatorname{div} \left(\frac{\nabla\phi(x)}{|\nabla\phi(x)|} \right)$$

LOCALIZED MEANS

$$\mu_{\text{in}} = \frac{\int_{\Omega_y} \mathcal{H}\phi(y) \cdot I(y) dy}{\int_{\Omega_y} \mathcal{H}\phi(y) dy}$$

$$\mu_{\text{out}} = \frac{\int_{\Omega_y} (1 - \mathcal{H}\phi(y)) \cdot I(y) dy}{\int_{\Omega_y} (1 - \mathcal{H}\phi(y)) dy}$$

LOCALIZED MEANS

$$\mu_{\text{in}}(x) = \frac{\int_{\Omega_y} \mathcal{B}(x, y) \cdot \mathcal{H}\phi(y) \cdot I(y) dy}{\int_{\Omega_y} \mathcal{B}(x, y) \cdot \mathcal{H}\phi(y) dy}$$

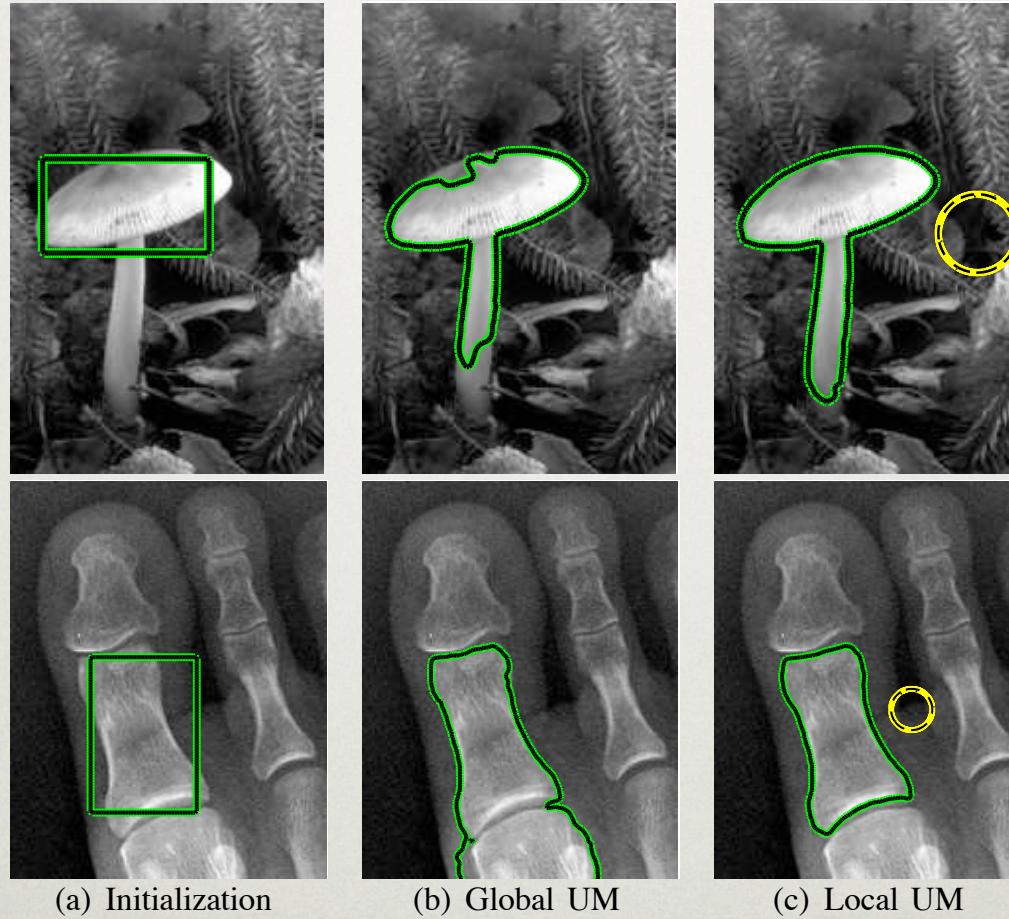
$$\mu_{\text{out}}(x) = \frac{\int_{\Omega_y} \mathcal{B}(x, y) \cdot (1 - \mathcal{H}\phi(y)) \cdot I(y) dy}{\int_{\Omega_y} \mathcal{B}(x, y) \cdot (1 - \mathcal{H}\phi(y)) dy}$$

UNIFORM MEAN MODEL

Assumption: The foreground and background will be approximately constant *locally*.

$$F_{\text{UM}} = \mathcal{H}\phi(y)(I(y) - \mu_{\text{in}}(x))^2 + (1 - \mathcal{H}\phi(y))(I(y) - \mu_{\text{out}}(x))^2$$

UNIFORM MEAN MODEL



(a) Initialization

(b) Global UM

(c) Local UM

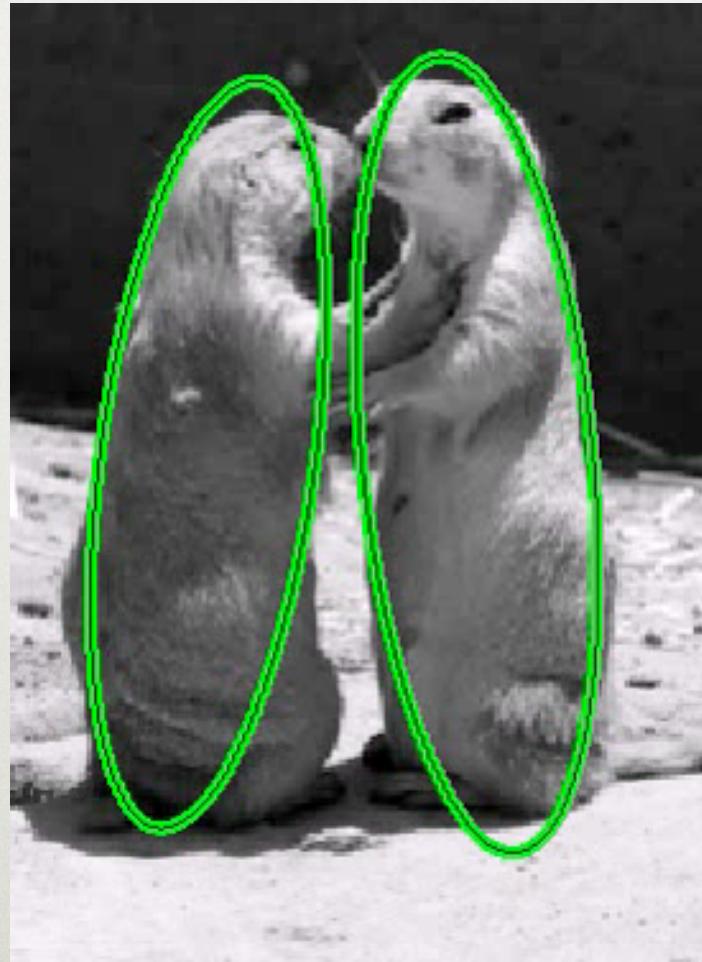
MEAN SEPARATION MODEL

Assumption: The foreground and background
should be very different *locally*.

$$F_{\text{MS}} = -(\mu_{\text{in}}(x) - \mu_{\text{out}}(x))^2$$

Yezzi *et al.* “A Fully Global Approach to Image Segmentation...,” JVCIR 2002

MEAN SEPARATION MODEL



PRELIMINARY RESEARCH

A WORD ON LOCALIZATION
FIBER BUNDLES
VESSEL ANALYSIS

BENEFITS OF LOCALIZATION

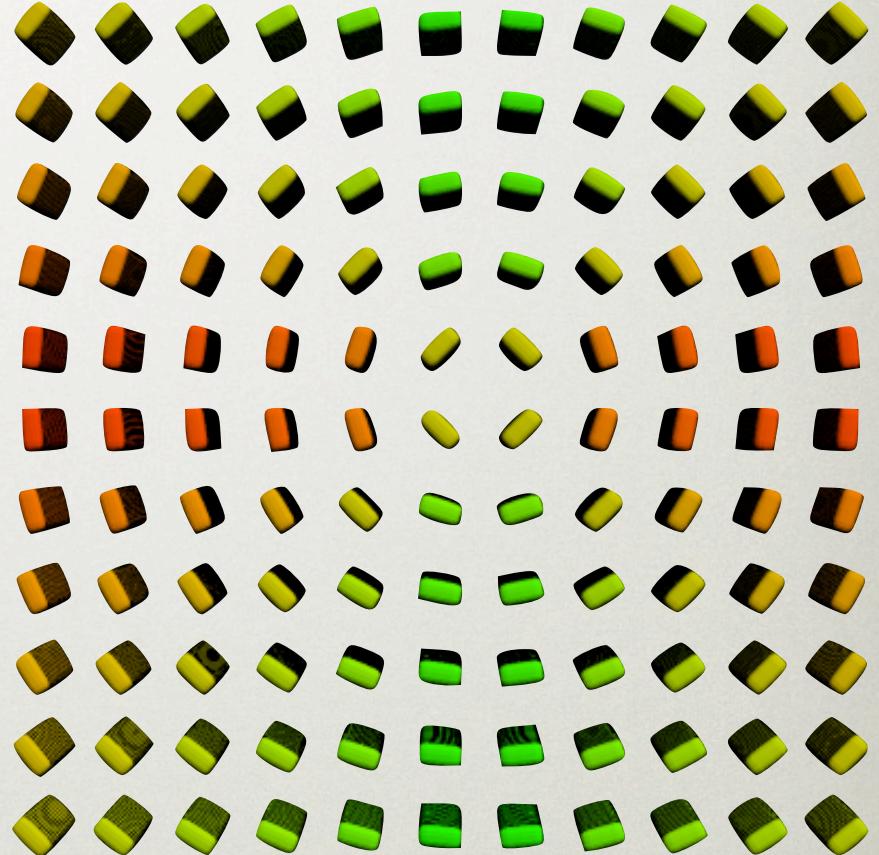
- Complex problems become simple
- Natural solution to many problems
- Scale is controllable

FIRST APPLICATIONS

- Fiber Bundle Segmentation
- Vessel Analysis

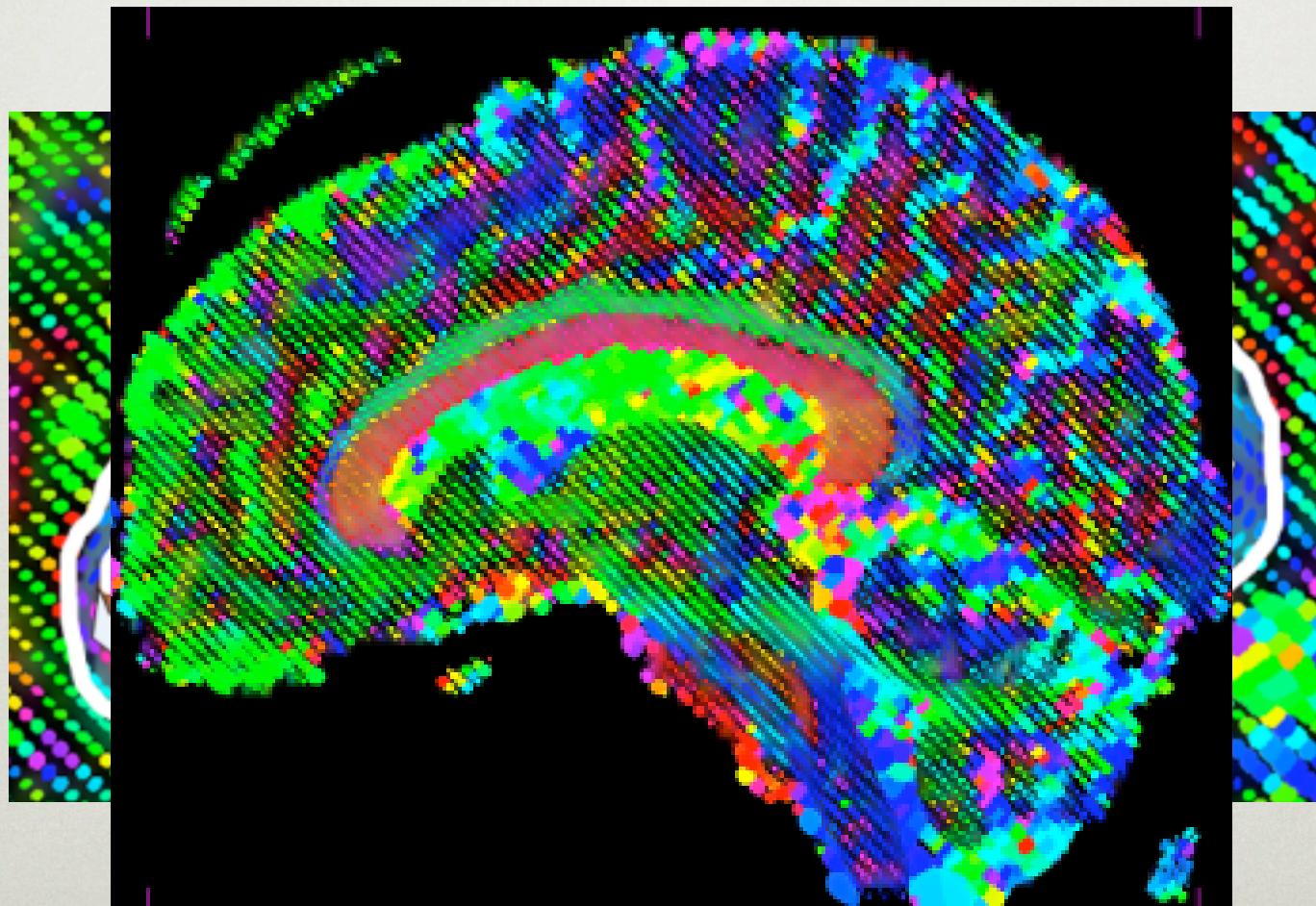
FIBER BUNDLES

- DW-MRI
- 3x3 Tensor Data
- Brain connectivity
- Analyze shape



Lankton *et al.* "Localized Statistics for DWI Fiber Bundle Segmentation," MMBIA, 2008

FIBER BUNDLES



FIBER BUNDLES

- Initialized with single fiber
- Evolve to capture full bundle
- Uses “tensor uniform mean model”

FIBER BUNDLES



VESSEL ANALYSIS

- Important
- Challenging
- Natural Solutions
- Segmentation
- Plaque Detection



Lankton *et al.* "Soft Plaque Detection...," MICCAI 2009 (*in submission*)

VESSEL SEGMENTATION

- CTA imagery
- Simple initialization
- No leaks
- Branch handling
- No shape information



VESSEL SEGMENTATION

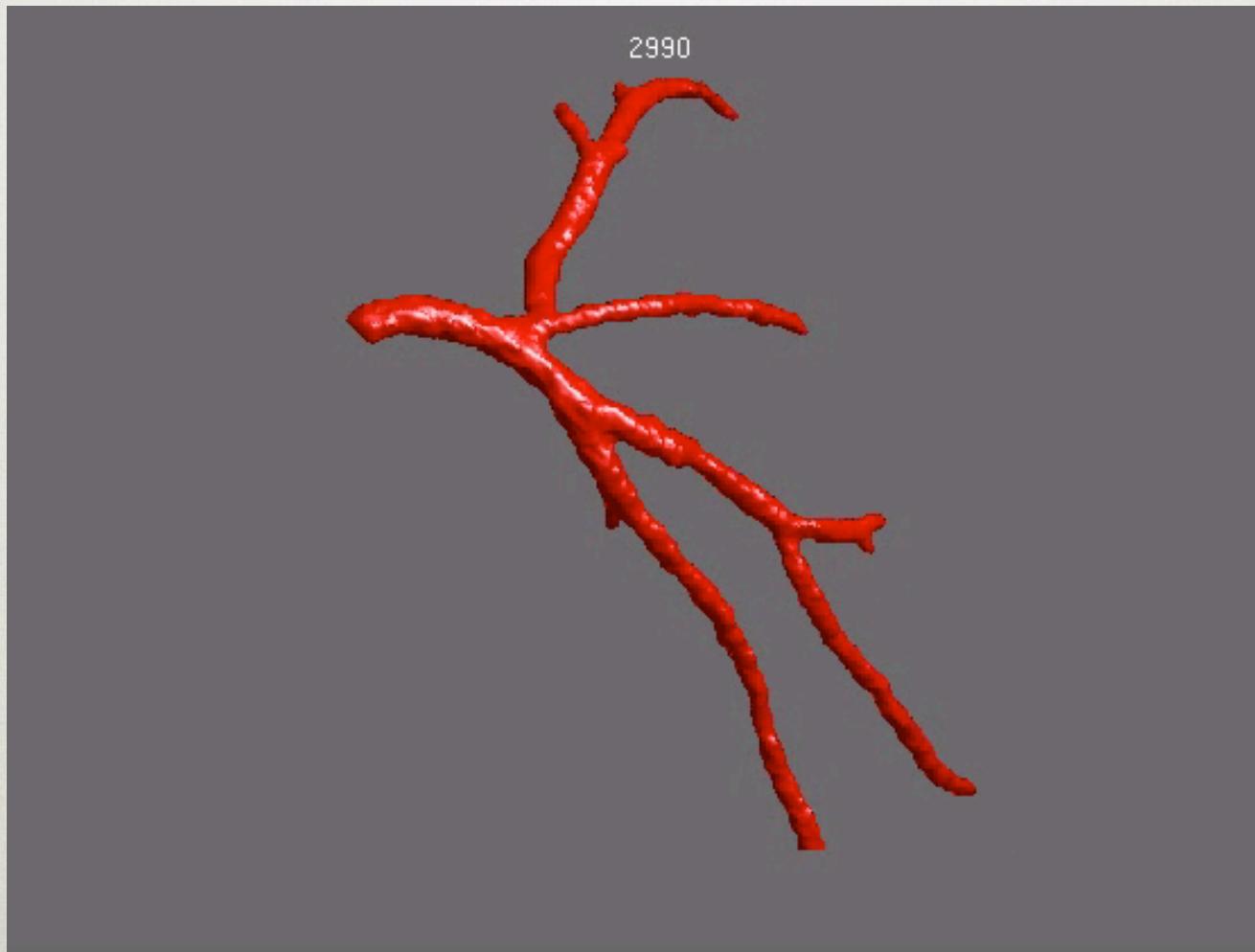
Localized Uniform Modeling Energy

$$F_{\text{UM}} = \mathcal{H}\phi(y)(I(y) - \mu_{\text{in}}(x))^2 + (1 - \mathcal{H}\phi(y))(I(y) - \mu_{\text{out}}(x))^2$$

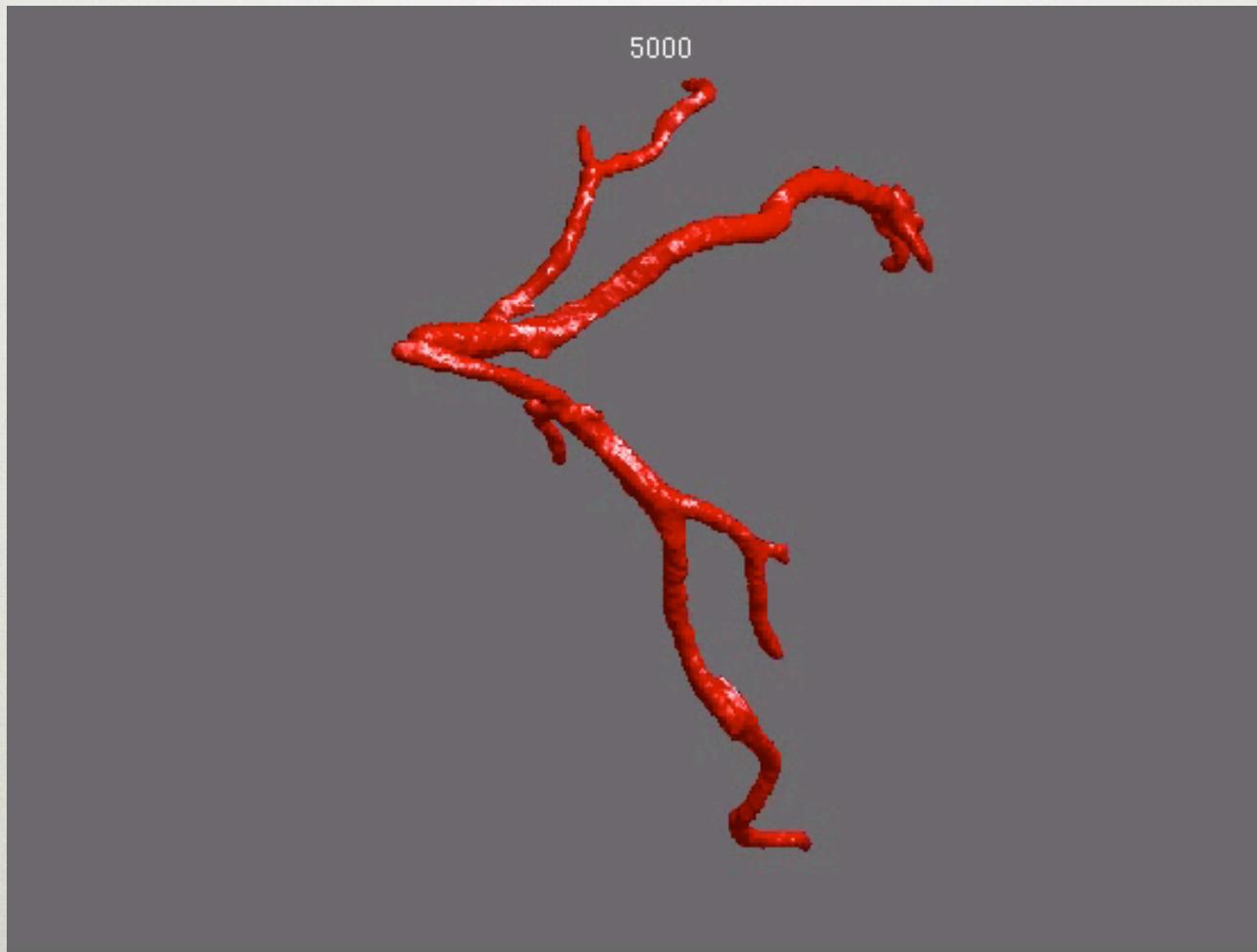
The Trick:

$$\tilde{\Omega} = \Omega \cap (I > \mu_{\text{HEART}} - 2\sigma_{\text{HEART}})$$

VESSEL SEGMENTATION

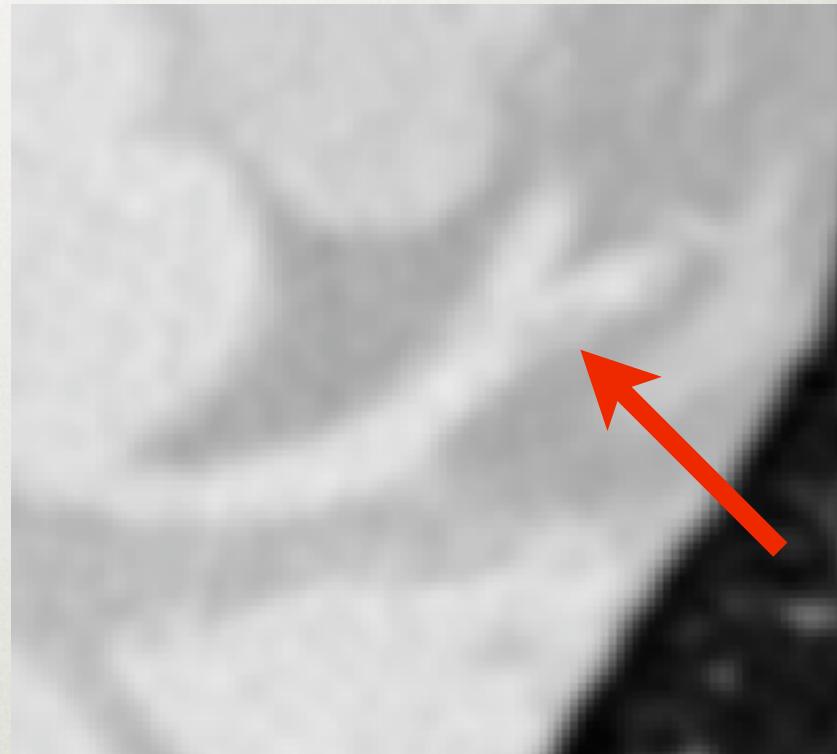


VESSEL SEGMENTATION



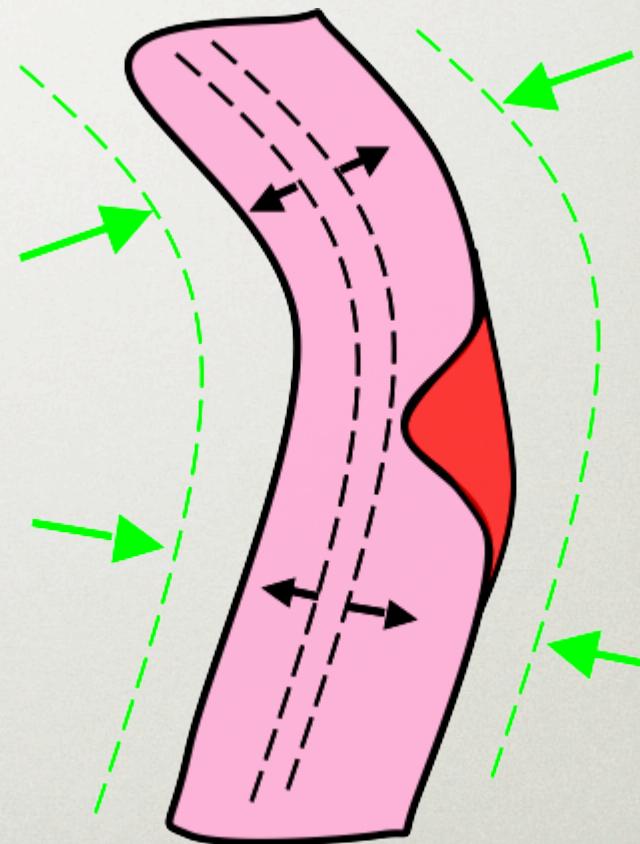
SOFT PLAQUE DETECTION

- Hard to see
- Very dangerous
- No good tools



SOFT PLAQUE DETECTION

- Two-front approach
- Inside moves out
- Outside moves in

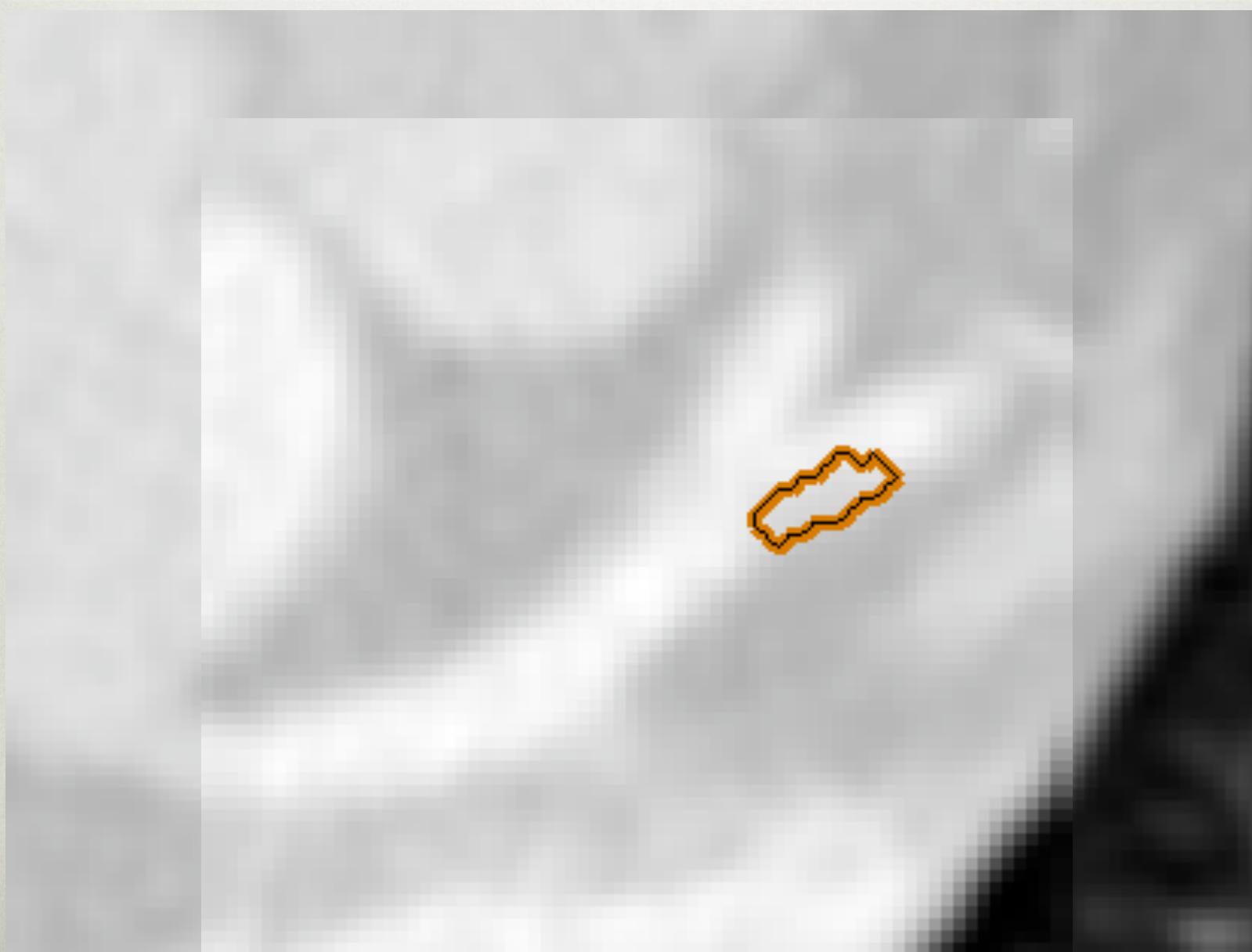


DETECTION ENERGY

Localized Means Separation Energy

$$F_{\text{MS}} = -(\mu_{\text{in}}(x) - \mu_{\text{out}}(x))^2$$

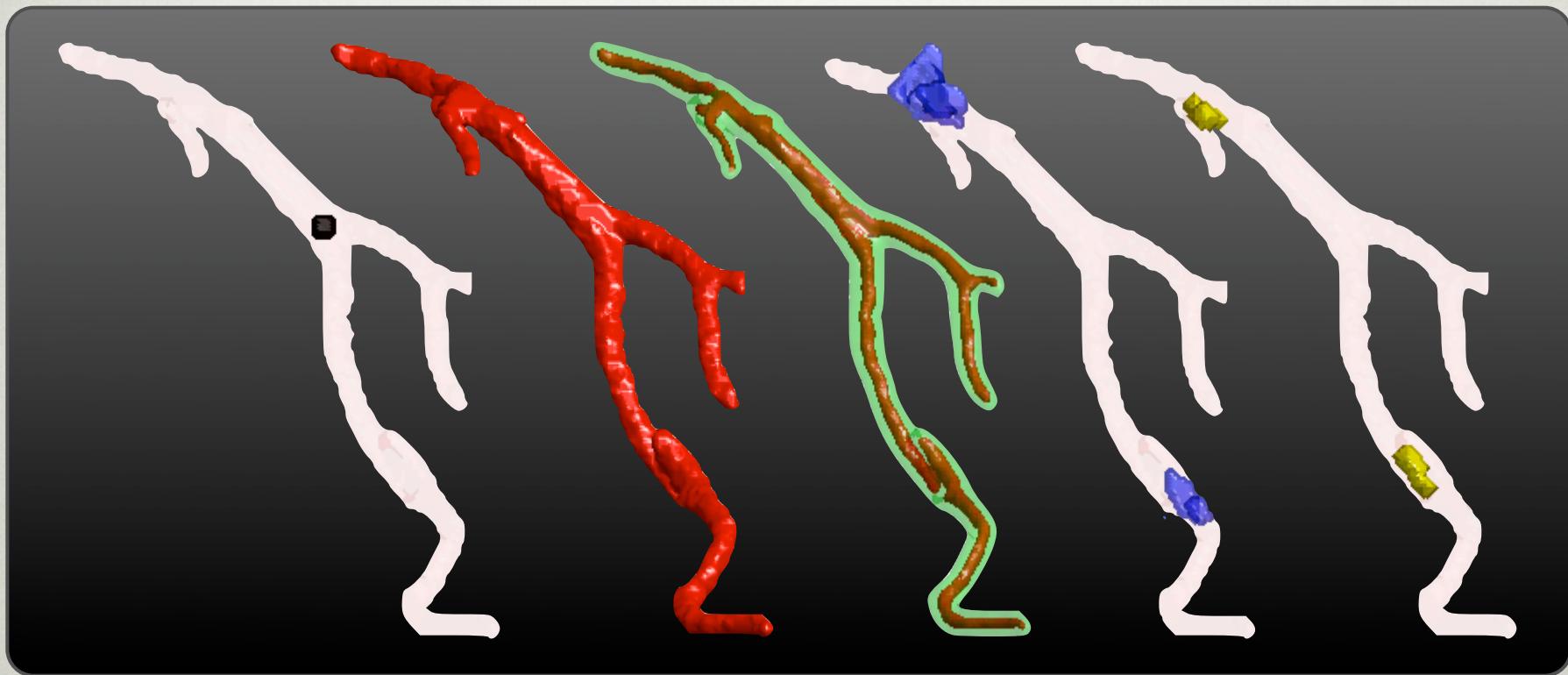
The Trick:
Clever Initializations



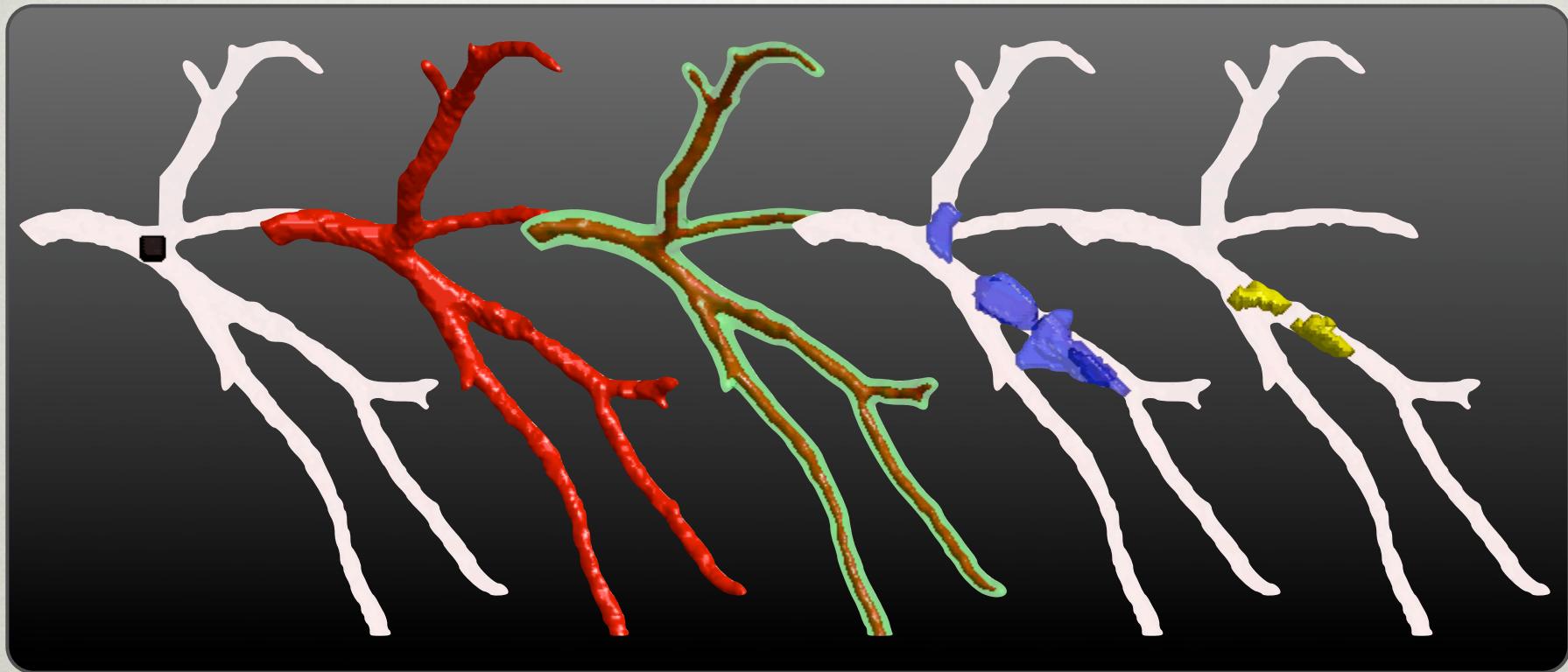
STEPS FOR DETECTION

- Segment the Vessel
- Create Initialization
- Segment In to Out
- Segment Out to In
- Check for Differences

NAÏVE RESULTS



NAÏVE RESULTS

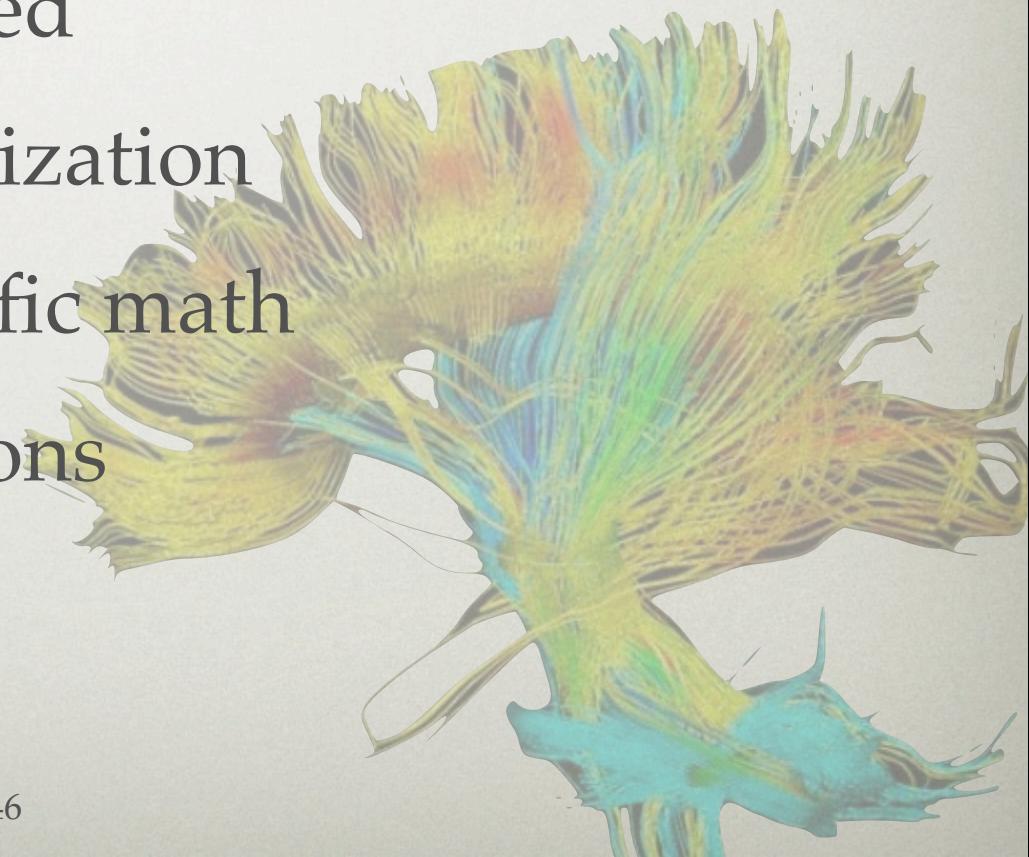


PROPOSED RESEARCH

FIBER BUNDLES
SOFT PLAQUE DETECTION
TEMPORAL LOCALIZATION

FIBER BUNDLES

- What we've learned
- Single-click Initialization
- More tensor-specific math
- Better segmentations



SOFT PLAQUE DETECTION

- Problems with naïve detection
- Coupling contours
- Improve robustness
- Larger studies



TEMPORAL LOCALIZATION



TEMPORAL LOCALIZATION



Lankton *et al.* "Tracking Through Changes in Scale," ICIP 2008

TIMELINE AND DELIVERABLES

KEY PUBLICATIONS

1. “**Localizing Region-Based Active Contours.**” S. Lankton and A. Tannenbaum. IEEE Transactions on Image Processing. Vol. 17, No. 11, pp 2029-2039, Nov. 2008.
2. “**Localized Statistics for DW-MRI Fiber Bundle Segmentation.**” S. Lankton, J. Melonakos, J. Malcolm, S. Dambreville, and A. Tannenbaum. Wkshp. Mathematical Methods in Biomedical Image Analysis. Jun. 2008.
3. “**Automatic Vessel Segmentation and Soft Plaque Detection.**” S. Lankton, A. Stillman, P. Raggi, A. Tannenbaum. Medical Imaging and Computer Assisted Intervention. 2009. (*in submission*)
4. “**Tracking Through Changes in Scale.**” S. Lankton, J. Malcolm, A. Nakhmani, and A. Tannenbaum. IEEE International Conference on Image Processing. pp. 241 - 244, Oct. 2008

ADDITIONAL PUBLICATIONS

1. “Statistical Shape Learning for 3D Tracking.” R. Sandhu, S. Lankton, S. Dambreville, A. Tannenbaum. CDC, 2009. (*in submission*)
2. “TAC: Thresholding Active Contours.” S. Dambreville, A. Yezzi, S. Lankton, and A. Tannenbaum. ICIP, 2008.
3. “Improved Tracking by Decoupling Target and Camera Motion.” S. Lankton and A. Tannenbaum. SPIE Electronic Imaging, 2008.
4. “Fast Optimal Mass Transport for Dynamic Active Contour Tracking on the GPU.” G. Pryor, T. Rehman, S. Lankton, P. Vela, and A. Tannenbaum. CDC, 2007.
5. “Hybrid Geodesic Region-Based Curve Evolutions for Image Segmentation.” S. Lankton, D. Nain, A. Yezzi, A. Tannenbaum. SPIE Medical Imaging, 2007.
6. “Fusion of IVUS and OCT Through Semi-Automatic Registration.” G. Unal, S. Lankton, S. Carlier, G. Slabuagh, and Y. Chen. MICCAI, 2006.

PLANNED PUBLICATIONS

1. **“Soft Plaque Detection and Vessel Analysis”**
IEEE Trans. in Medical Imaging. May

2. **“Temporally Localized Models for Tracking”**
IEEE Trans. in Pattern Recognition and Machine Intelligence. July

3. **“One-click Fiber Bundle Segmentation”**
TBD

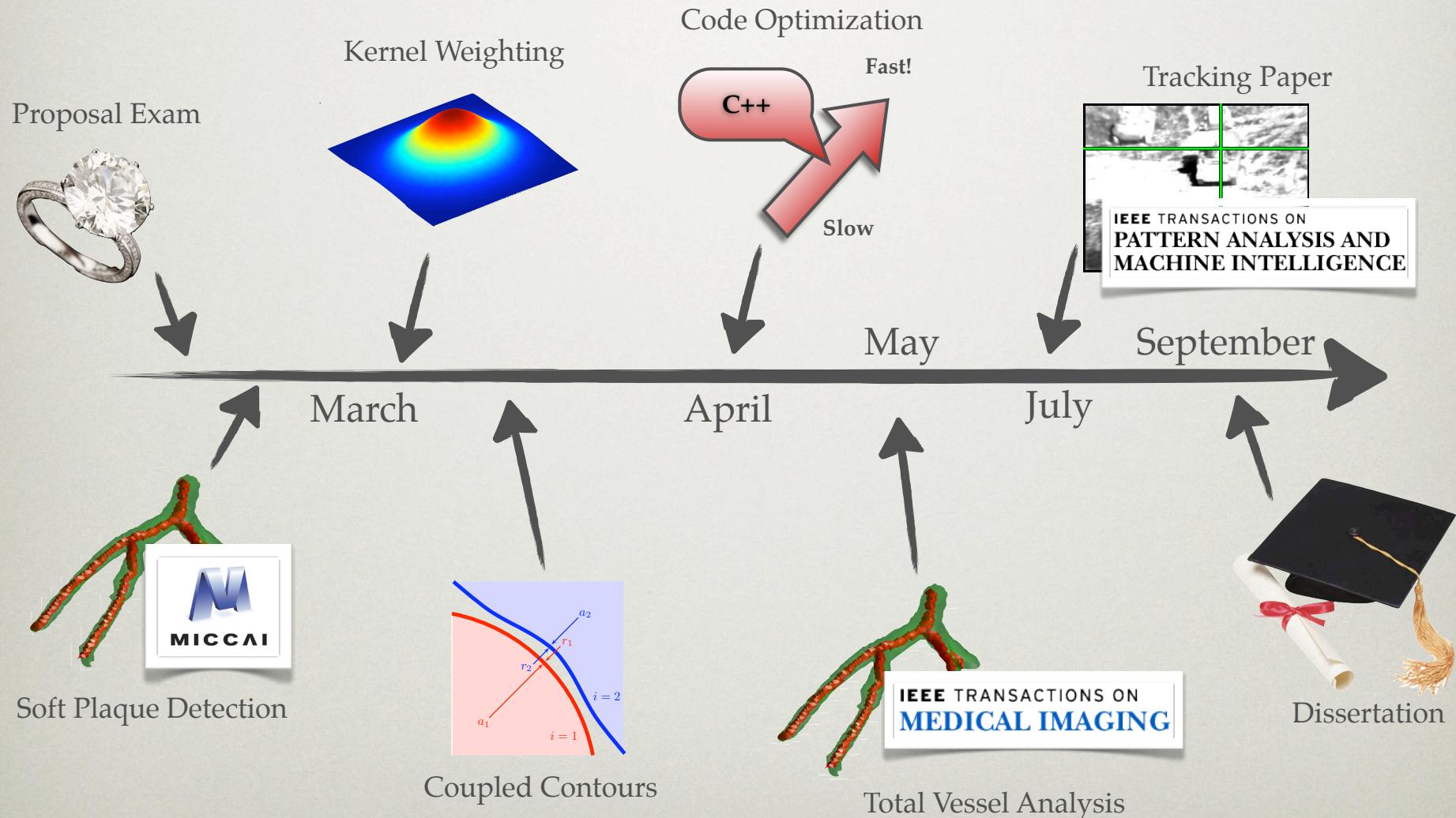
RESEARCH TIMELINE

Proposal Exam



Now

RESEARCH TIMELINE



THANK YOU.