









# INFLUENCE OF DRUG-POLYMER INTERACTIONS ON RELEASE KINETICS OF PLGA AND PLA/PEG NPS

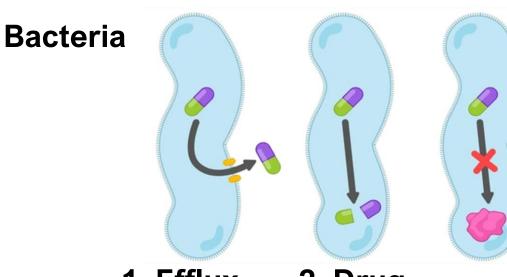
Merve Gul<sup>1,2</sup>, Ida Genta<sup>1</sup>, Maria M. Perez Madrigal<sup>2</sup>, Carlos Aleman<sup>2,3</sup>, Enrica Chiesa<sup>1</sup>

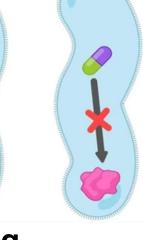
<sup>1</sup>Department of Drug Sciences, University of Pavia <sup>2</sup>Department of Chemical Engineering, Universitat Politècnica de Catalunya (UPC-EEBE) <sup>3</sup>Barcelona Research Center for Multiscale Science and Engineering, EEBE, Universitat Politècnica de Catalunya

## INTRODUCTION

Antimicrobial resistance (AMR) is a growing global health threat, requiring novel drug delivery strategies (1). Microfluidic-based synthesis of nano-sized carriers for drug delivery systems (NDDS) offers precise control over nanocarrier characteristics and improves encapsulation efficiency (2,3).

### (1) ANTIMICROBIAL RESISTANCE

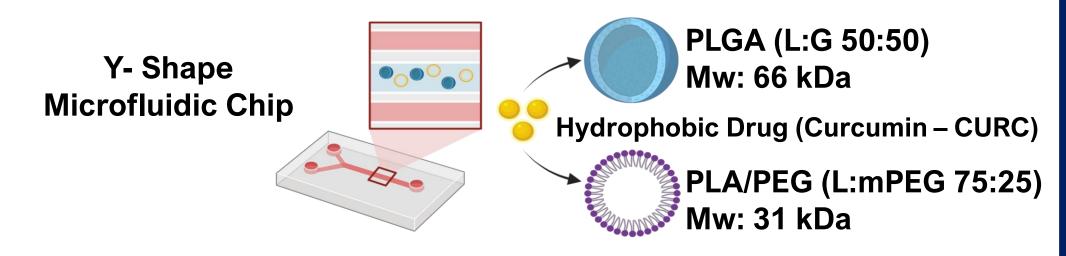




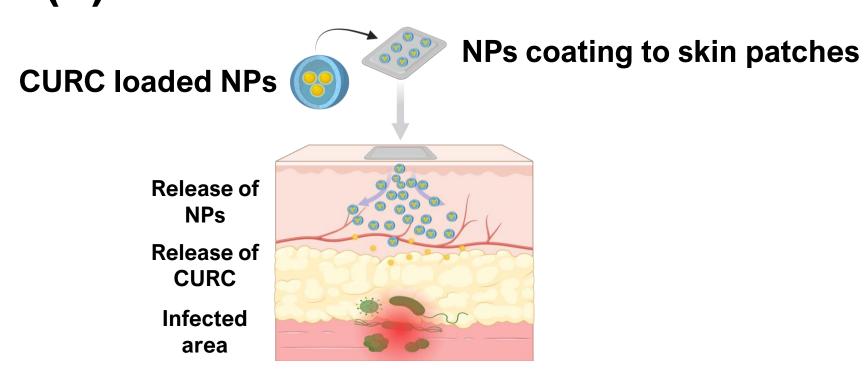
3. Mutation of Binding **Sides** 

2. Drug 1. Efflux Inhibition Pump

### (2) NPs SYNTHESIS BY MICROFLUIDICS



#### (3) DRUG DELIVERY SYSTEM



## **METHODS**

An ad hoc custom-built device was used, comprising a pumping module with two syringe pumps and an infusion setup designed to place a Passive Herringbone Mixer (PHBM) chip.

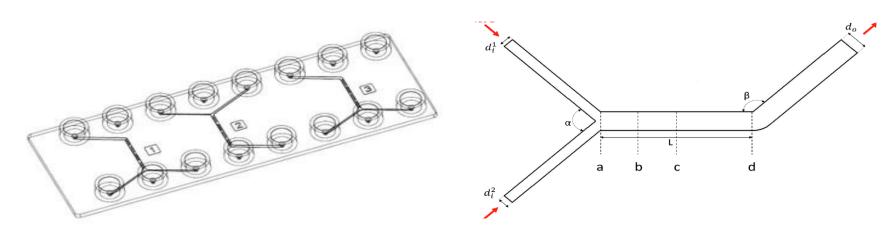


Figure 1: Representative scheme of a) outer and b) inner side of microfluidic chip (3).

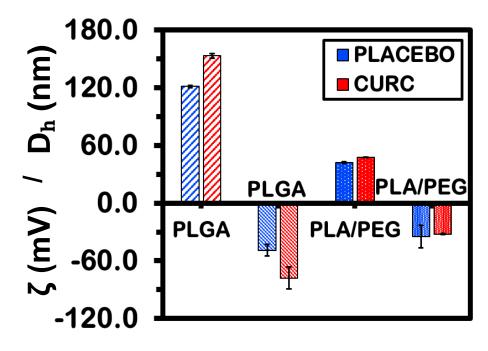
Table 1: Drug loading into NPs and micelles.

	Type of Syringes	Final Volume (mL)	Rate (TFR)	Flow Rate Ratio (FRR) (aqueous/
	<b>T</b>		(mL/min)	organic phase)
PLGA	Terumo 5 mL	2	8	4:1
NPs	Terumo 5 mL	2	8	4:1
PLA/PEG	Terumo 5 mL	2	3	3:1
NPs	Terumo 5 mL	2	3	3:1

## **RESULTS**

#### 1.Physical Properties of NPs

• NPs had uniform size distribution with PDI ≤ 0.2, consistent with TEM observations.



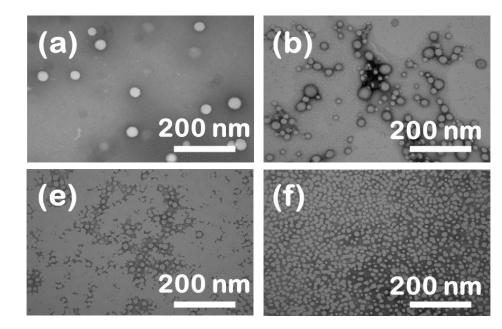


Figure 2: Physical features of PLGA NPs and PLA/PEG micelles.

Figure 3: TEM images of a) PLGA NPs, b) CURC loaded PLGA NPs, c) PLA-PEG micelles, and d) CURC loaded PLA-PEG micelles.

#### 2. Release Kinetics of NPs

Table 2: Drug loading into NPs and micelles.

	%		
Loading	PLGA	PLA/PEG	
Curcumin	61.91 ± 1.86	$13.74 \pm 0.97$	
	Payload ( % μg/mg)		
	2.81 ± 0.81	2.51 ± 0.57	
Highe Encapsul	ation 🚶	Slower Release	
Efficiency	(EE%)	Rate	

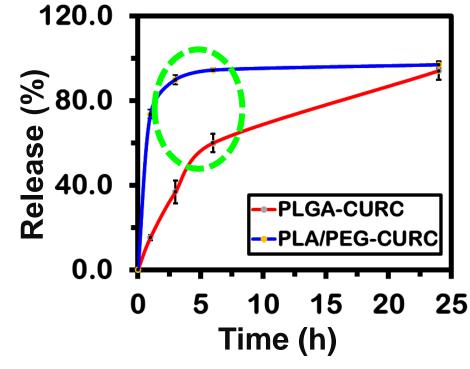
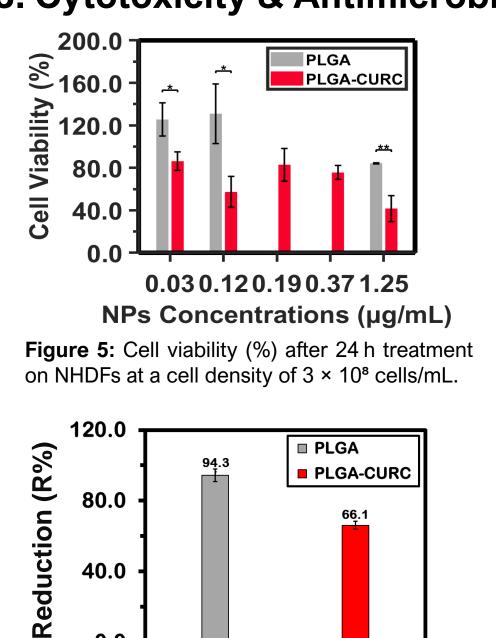
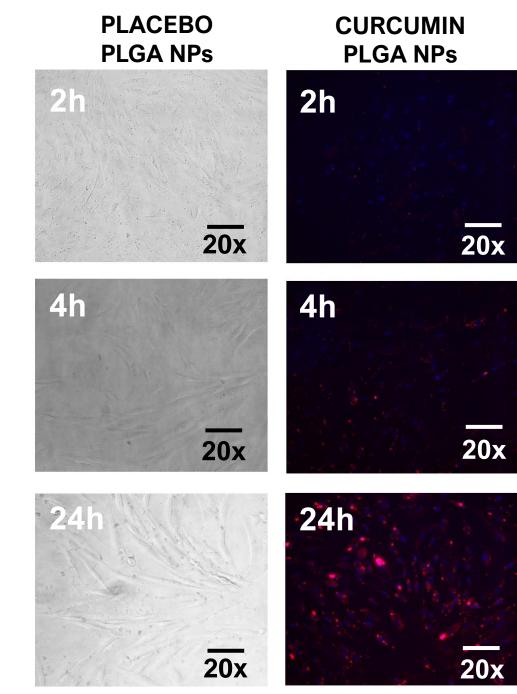


Figure 4: Release profiles of CURC from PLGA NPs and PLA/PEG micelles.

#### 3. Cytotoxicity & Antimicrobial Activity





Time (h) Figure 6: Bacterial reduction of S.epidermidis after 72h of treatment with CURC loaded PLGA NPs with a MIC of 0.1 mg/mL.

**PLGA-CURC** 

**PLGA** 

Figure 7: Fluorescence microscope images of placebo and CURC loaded PLGA NPs on NHDFs after 2, 4 and 24 h indicating cellular uptake.

## CONCLUSION

- CURC loaded PLGA NPs were better candidates for controlled drug delivery due to hydrophobic interactions between the drug and the polymer.
- No or slight cytotoxic effect of CURC NPs was observed on NHDFs with progressive cellular internalization of NPs.
- The choice of polymer composition plays a key role in drug-polymer interactions and release kinetics to achieve more controlled delivery and improved therapeutic efficacy in regenerative medicine.



- (1) Vega-Vásquez, P. et al. Front. Bioeng. Biotechnol. 2020, 8, 2296-4185.
- (2) Fu, Y. S. et al. *Biomed. Pharmacother*. 2021, 141, 111888. (3) Chiesa et al., International Journal of Pharmaceutics, Volume 629, 2022, 122368, ISSN 0378-5173.
- Acknowledgements

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