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**Reply:** We thank Dr. Beglinger and colleagues for their interest in our work (1).

On the basis of their own studies and of reports in the literature dealing with secretin and cholecystokinin (CCK), they assert that there is little evidence supporting the occurrence of potentiation of pancreatic enzyme secretion in vivo in dogs. This may hold true for secretin and CCK, but we reported on neurotensin, which may act quite differently.

Dr. Beglinger et al. criticize that we did not present data on maximal pancreatic protein secretion for the combined stimulation. As stated, however, we have tried to approach "physiological" hormone levels and, therefore, avoided high-peptide doses. Maximal pancreatic stimulation may yield interesting results, but our interest was not in a pharmacologic study.

Similarly, the lack of potentiation of bicarbonate output after the combination of CCK and secretin in our study may represent a dose-related phenomenon. Other investigators gave  $5 \text{ pmol} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$  as the smallest dose of secretin (2-4), whereas we used  $0.08 \text{ pmol} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$  (basis of this calculation was that  $3.6 \mu\text{g}$  of synthetic secretin represents 1 clinical unit).

We are sorry that our paragraph concerning methods was too short: the mean secretion ( $\bar{y}$ ) stimulated by the three doses of neurotensin given alone or in combination with secretin/CCK was calculated from the analysis of regression as proposed by Elashoff (5).

The mean secretion of a combination was then compared with the sum of the mean secretion stimulated by the three doses of neurotensin plus the secretion stimulated either by secretin, CCK, or secretin and CCK from the same dog using the paired two-tailed Student's *t*-test. Basal secretion was always subtracted.

We admit that the problem of "wash-out" is not completely solved. Although we observed no further reduction of protein output after the 30-min infusion of secretin, a small residuum of intraductular protein cannot be excluded. This protein would then be washed out by the flow elicited by neurotensin. It would add to the protein secreted in response to neurotensin. But the protein output observed under these circumstances was greater than additive. Two more facts minimized any washout of protein during the secretin/neurotensin combination: the wash-out phe-

nomenon is related to the ductular flow rate and the flow rate after the combination of secretin and neurotensin was identical ( $2.3 \text{ ml} \cdot 15 \text{ min}^{-1}$ ) with the added flow rates elicited by secretin and neurotensin each given alone.

Thus, while we agree that caution is needed, the evidence available points to a potentiation of pancreatic protein output in the dog when the combination of secretin and neurotensin is given in the doses described.

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### Galactose Clearance as a Measure of Hepatic Blood Flow

Dear Sir:

An improved assay for galactose has been used by Henderson et al. (1) to investigate the estimation of organ blood flow from organ clearance of a substance taken up by first-order kinetics (2), as applied to the estimation of the rate of blood flow through the liver from the hepatic clearance of galactose. Since the estimation is to be noninvasive (the hepatic vein is not to be sampled), it is highly model-dependent. Misunderstandings of the limitations of just this method have led, in the past, to notable errors in renal pathophysiology, such as the inference of severe renal ischemia in acute anuria (2). If such errors are to be avoided in hepatology, the kinetics underlying the limitations of the estimation must be made explicit. We propose to do this here, taking into account the fact that hepatic uptake of galactose follows Michaelis-Menten kinetics (3,4), whereby some of the questions raised by Henderson et al. (1) can be answered.

In this method, a steady infusion of galactose at the rate  $I$  is balanced by steady hepatic uptake; the resulting galactose concentrations,  $c_i$  upstream and  $c_o$  downstream of the liver, are also steady. Clearance is defined by  $Cl = I/\bar{c}_i$ , and extraction fraction by  $E = 1 - c_o/c_i$ . If  $F$  is the rate of hepatic blood flow that is to be estimated, we can write Fick's principle,  $I = F(c_i - c_o)$ , in the form

$$\text{Clearance} = FE \leq F, \quad (1)$$

where the last relation follows from  $E \leq 1$ . In the noninvasive method, one does not ascertain how much clearance falls short of  $F$  in each individual case because  $c_o$  (and hence  $E$ ) is not measured. We therefore consider this shortfall theoretically by

using the sinusoidal perfusion model of hepatic uptake. We begin with the undistributed version of the model (5,6).

The theoretical relation between clearance,  $F$ , and  $I$  is (5):

$$\text{Clearance} = F - F \exp\left(-\frac{V_{\max} - I}{FK_m}\right), \quad (2)$$

where  $V_{\max}$  is the maximum rate of galactose uptake by the liver at saturation, and  $K_m$  is the half-saturation (Michaelis) constant. The rate-limiting step in the hepatic uptake of galactose is phosphorylation by galactokinase (3) and the value of  $K_m$  is known to be 0.03–0.04 mg/ml from in vitro (7) and in vivo (3,5) studies. Typical  $V_{\max}$  of the normal human liver is 200–400 mg/min, but it can fall below 100 mg/min in liver disease (8) when extrahepatic elimination of galactose is taken into account. The infusion rates used by Henderson et al. (1), 25–100 mg/min, were smaller in each case than  $V_{\max}$  (otherwise, a steady state could not be reached). The resulting values of  $c_i$  were all either of the order of  $K_m$  or larger, while most values of  $c_o$  were below  $K_m$  (1). Hence, the arterial–venous difference  $c_i - c_o$  traversed most of the Michaelis–Menten range of elimination kinetics, and only the perivenous hepatocytes operated in the limit of first-order kinetics ( $c_o \ll K_m$ ). Data presented by Henderson et al. (1) do not suffice for the calculation of  $V_{\max}$ ,  $K_m$ , and  $F$  from Eq. (2), but the insertion in Eq. (2) of the aforementioned typical values readily reproduces the main features of the data. For example, the question was raised by Henderson et al. (1) as to why the doubling of  $I$  from initial values in the range 22–55 mg/min resulted in reductions in clearance, which averaged 8% in 14 subjects. Such a reduction is accomplished according to Eq. (2), if we set, for example,  $V_{\max} = 200$  mg/min,  $K_m = 0.035$  mg/ml, and  $F = 1500$  ml/min. Then Eq. (2) predicts clearance =  $0.95F = 1425$  ml/min for  $I = 45$  mg/min, and clearance =  $0.88F = 1320$  ml/min for  $I = 90$  mg/min (a drop in clearance of ~8%).

We now turn to the central question: under what conditions in clearance a good or bad estimate of  $F$ ? Clearance approaches  $F$  from below as the exponential factor in Eq. (2) is diminished; that is, as the fraction  $(V_{\max} - I)/FK_m$  is increased. Clearance will be >95% of  $F$  when that fraction is >3, and <80% of  $F$  when the fraction is <1.5. The former case has been exemplified earlier with  $I = 45$  mg/min. The latter case is illustrated by the same example if we reduce  $V_{\max}$  to 120 mg/min. This shows how rapidly clearance can fall below  $F$  with falling  $V_{\max}$ . In general terms, clearance is a good estimate of  $F$  at low  $F$  and high  $V_{\max}$ , and a poor one at high  $F$  and low  $V_{\max}$  (in liver disease). Reducing  $I$  in order to approach first-order (linear) kinetics, ( $I \ll V_{\max}$ ) brings clearance closer to  $F$ , but not decisively so:  $(V_{\max} - I)/FK_m$  may be small even for negligible  $I$ , and large even for  $I$  comparable with  $V_{\max}$ . In the latter case, clearance  $\approx F$  will be independent of  $I$  (equivalently, of  $c_i$ ) even when many (periportal) hepatocytes operate in the nonlinear range of Michaelis–Menten kinetics. Then, despite that nonlinearity, the ratio of dose to area under the  $c_i(t)$  curve obtained in a transient measurement will give the same value of clearance as  $I/c_i$  in the steady-state measurement on the same subject (1).

The foregoing discussion in terms of Eq. (2) is oversimplified. Consider an intrahepatic shunt, through which some part  $pF$  ( $0 < p < 1$ ) of the flow rate  $F$  carries the concentration  $c_i$  undiminished into the vein. Suppose also that the substrate is eliminated completely, in one pass through the liver, from the remaining part  $(1 - p)F$  of the flow. Then  $E = 1 - p$ , and clearance =  $(1 - p)F$ , which is independent of  $I$  [so that such cannot be the case (1) discussed earlier]. We see that clearance only estimates the flow rate  $(1 - p)F$  through the enzymatically active part of the liver, and that is satisfactory. But what if the shunt is replaced by a vascular pathway of flow rate  $pF$  associated with some  $qV_{\max}$  ( $0 < q < 1$ ), leaving the remainder of the liver with  $(1 - q)V_{\max}$ ? We must then use Eq. (2) separately for each part of the liver. Since  $c_i$

is common to both parts, and since the appropriate partial infusion rates are  $pI$  and  $(1 - p)I$ , the total clearance will be the sum of the two clearances so calculated. If  $p = q$ , we recover readily Eq. (2) for the complete liver, but one can show that whenever  $p \neq q$ , the resulting clearance is always less than at  $p = q$ . For example, if we take the first of the foregoing examples (with  $I = 45$  mg/min) and choose  $p = 1/3$  and  $q = 2/3$ , we find clearance =  $0.85F$  (in place of clearance =  $0.95F$ ).

Proceeding in this way to consider a set of vascular pathways, we arrive at the distributed model of hepatic uptake [(9) and references therein], for which there is the general result: any heterogeneity of extraction in a set of parallel vascular pathways (without change in the total organ  $V_{\max}$ ,  $F$ ,  $K_m$ ) must diminish the organ extraction fraction  $E$ , and hence also clearance by Eq. (1). For a real liver, there is therefore an additional determinant of the accuracy of the estimation of  $F$  by clearance: the greater the heterogeneity of extraction [which can be quantified precisely (9)], the farther does the clearance  $Cl$  fall below the rate  $F$  of hepatic blood flow.

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**Reply:** In response to the letter from Keiding and Bass concerning our paper "First-order clearance of plasma galactose: the effect of liver disease" in *GASTROENTEROLOGY* 1982;83:1090–6, we would make the following points.

We agree that it is important to understand the limitations of clearance methodology in applying such to blood flow estimation. While we accept their model for galactose elimination, and acknowledge the group's enormous contribution in this field, we do not agree with their typical values applied to this theoretical model. First, the normal  $V_{\max}$  from their own source is  $406 \pm 91$  mg/min; in more than cirrhotic patients we have found only 2 patients with a value <150 mg/min. Second, the reported  $K_m$

values for galactokinase vary from 0.017 to 0.036 mg/ml in animal studies, and in human studies galactokinase has been purified with a  $K_m = 0.018\text{--}0.027$  mg/ml (1). The limits of the rates of liver blood flow ( $F$ ), in normal subjects and patients with liver disease, lie between 500 and 2000 ml/min. When these parameter values (which are within acceptable pathophysiologic limits), are used in Eq. (2) at  $I = 45$  mg/min, clearance is, at worst,  $\sim 0.94F$  for  $F = 2000$ ,  $V_{\max} = 250$ , and  $K_m = 0.036$ . The theoretical example they cite to explain the 8% drop in clearance with a twofold increase in  $I$  is, we believe, based on an unrealistic combination of  $V_{\max}$  and  $F$ . The clearance-to- $V_{\max}$  ratio of galactose usually lies in the 3:1 or 4:1 range (2,3), and although this will vary with different liver diseases, we have never measured the 7.5:1 ratio they suggest. While increasing the infusion rate will contribute to the clearance reduction by the mechanism they suggest, we submit that the full explanation is more complex.

In response to their question as to what conditions are required to best estimate flow by a clearance method, we would add the following. Substitution of the cited values of  $V_{\max}$  and  $K_m$  for normal subjects satisfies the criteria of  $(V_{\max} - I)/FK_m > 3$ ; in patients with advanced liver disease (e.g., a  $V_{\max} = 150$  mg/min, flow maintained at 1000 ml/min),  $(V_{\max} - I)/FK_m > 2.92$ , i.e., clearance still approximates flow. On a theoretical basis, Keiding and Bass undersell the capability of galactose clearance to approximate liver blood flow. The practical application of the method in advanced liver disease, as presented in our paper, negates their theoretical argument.

Finally, the limitations of the oversimplification must be recog-

nized, particularly in respect to intrahepatic shunting. Total liver blood flow cannot be measured by a clearance method without knowing hepatic extraction, which may well vary in different parts of the liver. Any clearance method applied without hepatic vein catheterization and within the constraints outlined previously has the limitation of measuring flow to functioning liver tissue: this is the important flow metabolically. The data presented in our paper, and reinforced by the preceding examples, show that galactose clearance at these concentrations approaches the ideal of measuring functional liver blood flow.

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