

Biomarker estimation from medical images: segmentation-based and segmentation-free approaches

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Biomarker

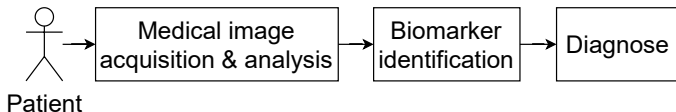
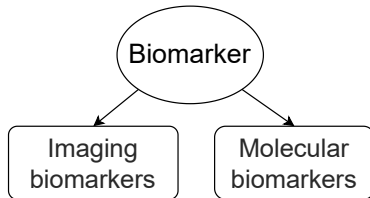
A biomarker is anything that can be used as an indicator of a particular disease state.

concept

category

develop

apply



Biomarker

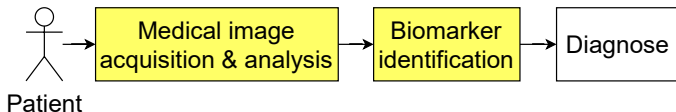
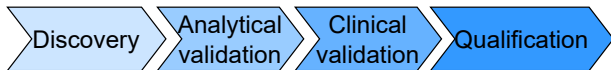
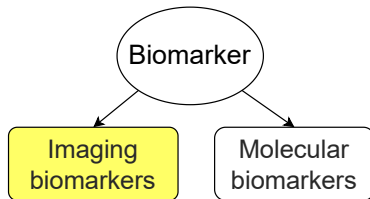
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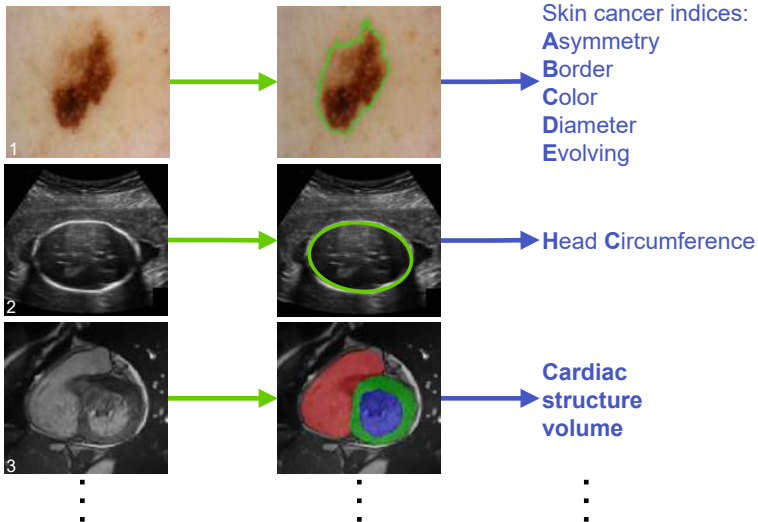


Generally...

How to measure a **biomarker**?



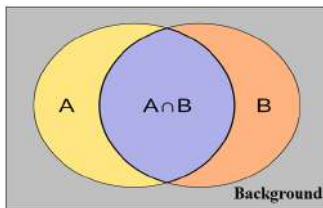
Biomarker identification examples

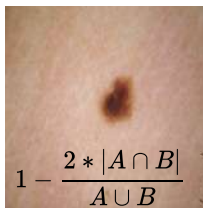


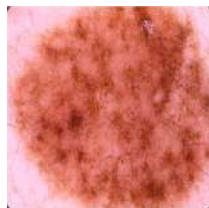
Problems



Segmentation: 😞 Intermediate step, prone to errors

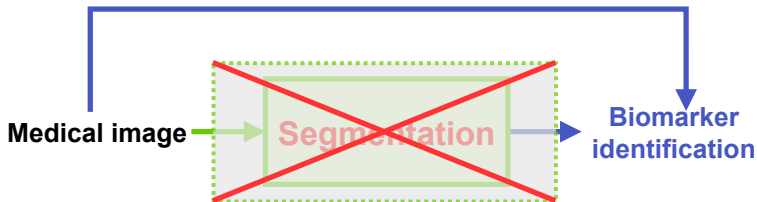



$$1 - \frac{2 * |A \cap B|}{A \cup B}$$



Dice loss in Deep learning: 😞 Does not generalize well

Very recently...



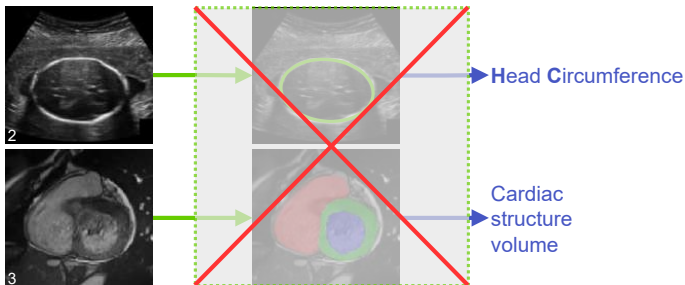
Direct estimation methods:

- 😊 Without segmentation intervention
- 😞 Less explainable

Contributions

Biomarker estimation:

- Segmentation-based -----
 - ① **New Kappa loss function** VS
- Segmentation-free (novel) -----
 - ② **Direct** biomarker estimation **without segmentation**
 - ③ **Explainability** of segmentation-free models



Thesis outline

Introduction

Kappa loss

HC estimation

HC estimation
Explainability

Cardiac volume

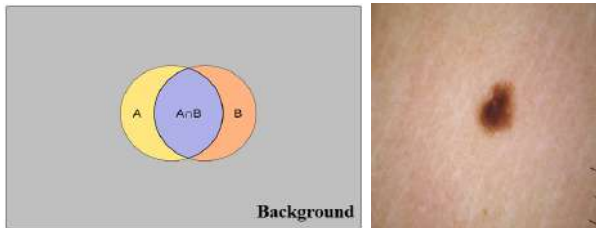
Conclusions

- ② Kappa loss for skin lesion segmentation [Chapter 3]
- ③ Direct fetus head circumference estimation [Chapter 4]
 - HC estimation via Seg vs. Seg-free
 - Explainability for regression CNN
- ④ Direct cardiac structure volume prediction [Chapter 5]
- ⑤ Conclusions and Perspectives [Chapter 6]

Kappa loss for skin lesion segmentation in fully convolutional network

Dice loss

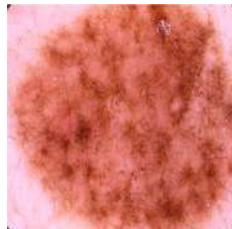
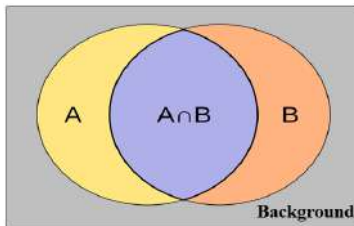
Class imbalance problem



$$\text{Dice metric} = \frac{2 * |A \cap B|}{A \cup B} \quad (1)$$

Dice loss

Problem: When classes are balanced



$$\text{Dice loss} = 1 - \frac{2 \sum_{i=1}^N p_i g_i}{\sum_{i=1}^N (p_i + g_i)} \quad (2)$$

☹ Background is discarded in Dice loss!

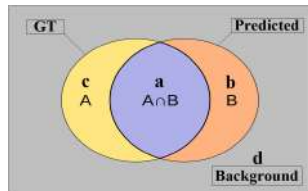
p_i : probability of predicted pixels;

g_i : ground truth pixels.

Kappa index

□ **Kappa index** (Cohen, 1960): the agreement between two raters.

		GT (Rater 1)		
		+	-	Total
Predicted results (Rater 2)	+	a	b	$a + b$
	-	c	d	$c + d$
Total		$a + c$	$b + d$	N



$$\kappa = \frac{2(ad - bc)}{(a + b)(b + d) + (a + c)(c + d)} \quad (3)$$

When $d \gg (a; b; c)$, Eq (3) becomes:

$$\lim_{d \rightarrow \infty} \kappa = \frac{2a}{2a + b + c} \rightarrow \text{Dice}$$

Experimental results

- **Datasets:** Skin lesion (6), data augmentation
- **Segmentation Model:** U-Net, train from scratch
- **Loss functions:** Dice loss; Kappa loss
- **Evaluation metrics:** Dice index \uparrow ; Hausdorff distance \downarrow

dataset(#)	Dice loss		Kappa loss	
	DI \uparrow	HD \downarrow	DI \uparrow	HD \downarrow
Non-mel(87) \dagger	0.65 \pm 0.11	5.06 \pm 1.79	0.73 \pm 0.11	4.70 \pm 2.02
Mel(119) \dagger	0.80 \pm 0.06	6.70 \pm 1.93	0.81 \pm 0.03	6.59 \pm 1.88
SCD(206) \dagger	0.82 \pm 0.04	7.94 \pm 1.72	0.83 \pm 0.03	7.91 \pm 1.68
ISIC-16(900) \diamond	0.80 \pm 0.05	8.42 \pm 2.19	0.84 \pm 0.01	8.41 \pm 2.25
ISIC-17(2000) \diamond	0.80 \pm 0.05	8.07 \pm 1.93	0.84 \pm 0.05	8.03 \pm 1.94
ISIC-18(2594) \diamond	0.81 \pm 0.03	7.59 \pm 2.60	0.82 \pm 0.04	7.52 \pm 2.66

✓ Kappa loss $>$ Dice loss

- Input data & scale

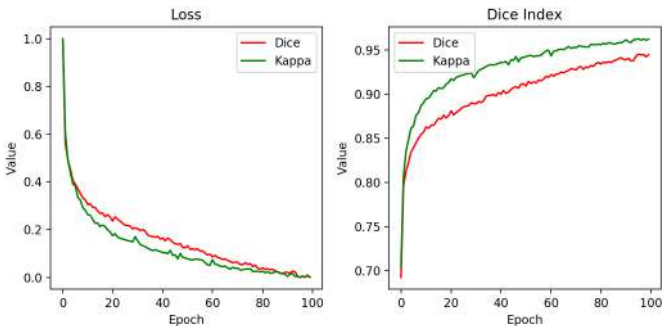
\dagger Skin-Cancer-Detection (SCD, Non-mel, Mel):

<https://uwaterloo.ca/vision-image-processing-lab/research-demos/skin-cancer-detection>

\diamond International Skin Imaging Collaboration (ISIC):

<https://www.isic-archive.com/#!/topWithHeader/wideContentTop/main>

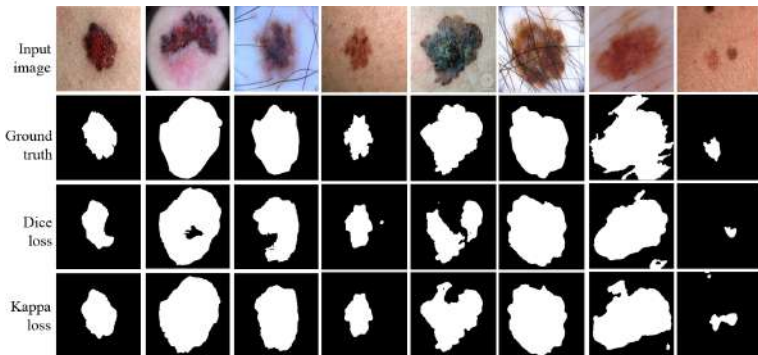
Learning curve



Loss curve (left) and Dice index (right) of training process:

- ❑ **Convergence:** Kappa loss (green) > Dice loss (red);
- ❑ **Dice index:** Kappa loss (green) > Dice loss (red).

Qualitative results



✗ Dice loss: Defects/holes in the skin lesion.

✓ Kappa loss: Less segmentation error.

Summary of Kappa loss

- ❑ Takes into account all the pixels → more accurate.
- ❑ Kappa loss is generalization of Dice loss.
- ❑ Performs as good as Dice loss → background information.
- ❑ Segmentation results as prerequisite for biomarker identification → direct estimation.

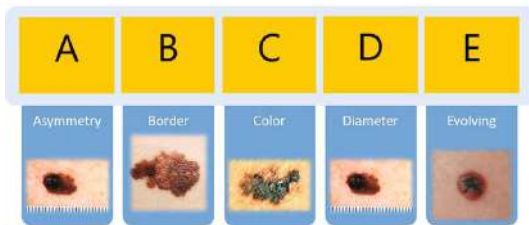
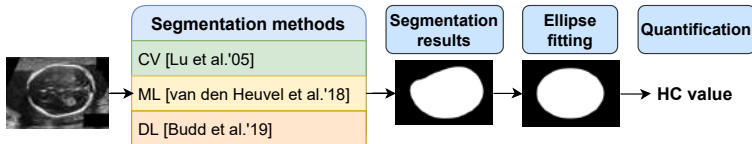


Image credit: <https://doi.org/10.1007/s11063-020-10364-y>

Direct fetus head circumference (HC) estimation from ultrasound images

Related works

➤ HC measurements → **Segmentation** (State-of-the-art):



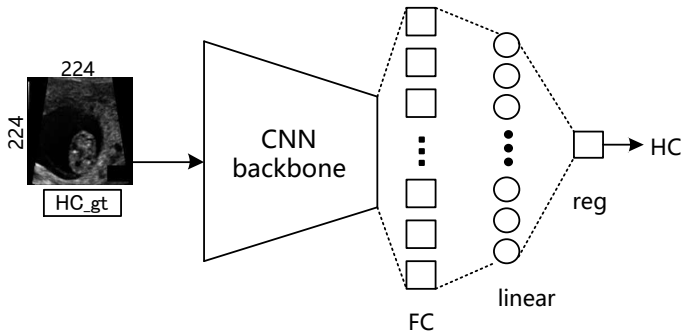
✓ **Pros:** Have segmentation results, **explainable**.

✗ **Cons:** Multi steps(Seg+ellipse fitting), prone to errors.

➤ Direct measurements → **Regression** methods:

- Head pose, facial landmark (Riegler et al., 2013)
- Left ventricular volumes prediction (Luo et al., 2016)
- Kidney volume prediction (Hussain et al., 2016)
- Brain age (Li et al., 2018)

Proposed Regression CNN



Benefits of proposed method:

- Doesn't need ground truth images, **no segmentation errors**.
- Can estimate the HC value **directly**.

Proposed regression CNN

2 changes from classification CNN to regression CNN model:

- ~~Softmax layer~~ → **Linear regression layer**
- ~~Classification loss~~ → **Regression loss**

$$- MAE = \frac{1}{n} \sum_{i=1}^n |p_i - g_i|$$

$$- MSE = \frac{1}{n} \sum_{i=1}^n (p_i - g_i)^2$$

$$- HL^* = \begin{cases} \frac{1}{n} \sum_{i=1}^n \frac{1}{2} (p_i - g_i)^2, & \text{for } |p_i - g_i| < \delta \\ \frac{1}{n} \sum_{i=1}^n \delta * (|p_i - g_i| - \frac{\delta}{2}), & \text{otherwise} \end{cases}$$

*HL: Huber Loss;

p_i = predicted values;

g_i = ground truth values

Experiment protocol

Models

- Segmentation models+CNN backbones, Dice loss
- Regression models+CNN backbones, MAE, MSE, HL loss
- Transfer learning: pretrained on ImageNet[†], fine-tuned on HC18.

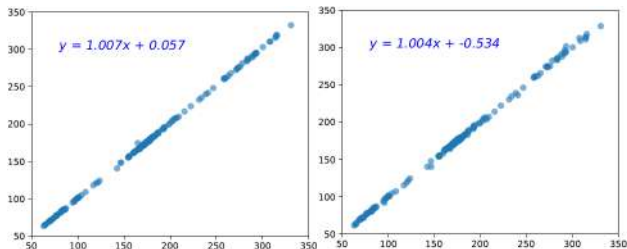
Settings

- HC18[‡] dataset, 5-fold cross validation
- Preprocessing: Data augmentation, Normalization, Resizing
- Metrics: MAE, percentage of MAE (PMAE)

[†] <https://www.image-net.org/>

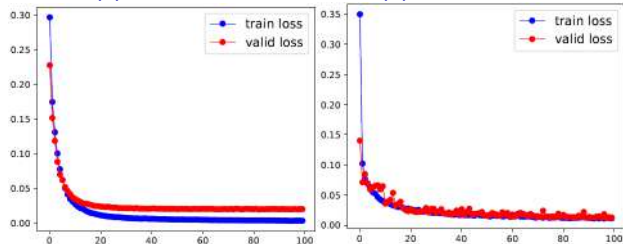
[‡] <https://hc18.grand-challenge.org/>

Qualitative analysis: Seg-based vs. Seg-free



(a) U-Net-B2

(b) Regression-B3



(c) U-Net-B2

(d) Regression-B3

Summary of HC estimation

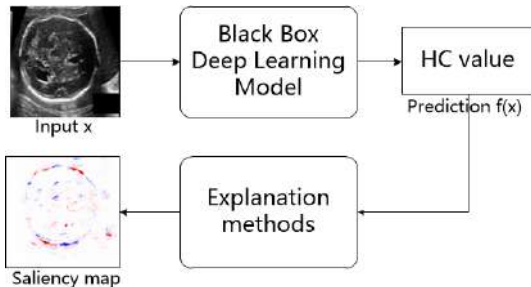
- ❑ Proposing **regression CNN model** → **directly estimate the HC value without segmentation intervention.**
- ❑ Evaluating Seg-based vs. Seg-free methods **fairly.**
- ❑ **Trade off** between prediction error and computation efficiency.
- ❑ Limitation: **Less explainable.**



[Journal of Imaging'22]

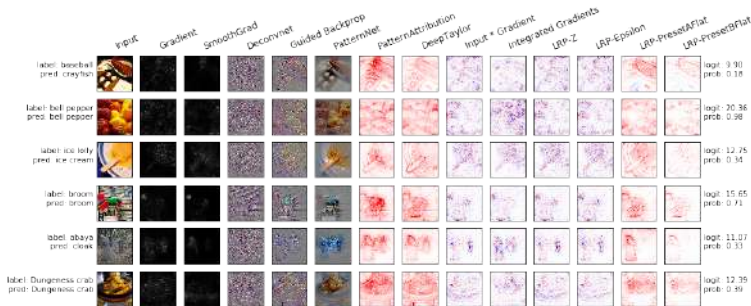
🔗 <https://github.com/jizhang02/HC-reg-seg>

Explainability for regression CNN



Saliency maps: Highlight features that model learns from images

- Verify prediction results
- Find out flaws and biases



Saliency maps of classification modelst.

Explanation methods:

Gradient

- Gradient¹
- SmoothGrad²
- Input*Gradient³

Deconvolution

- Integrated Gradients⁴
- DeConvNet⁵
- Guided BackProp⁶

LRP var.

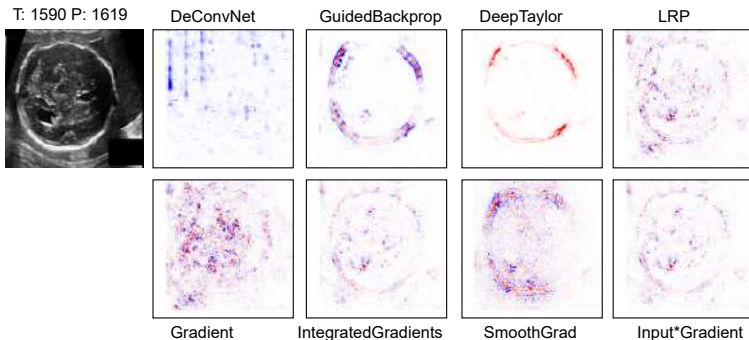
- LRP⁷
- DeepTayor⁸

Which method is suitable?

†Image credit: <https://github.com/albermax/investigate>

1.Simonyan et al., 2014; 2.Smilkov et al., 2017; 3.Shrikumar et al., 2016; 4.Sundararajan et al., 2017; 5.Zeiler et al., 2014; 6.Springenberg et al., 2015; 7. Layer-wise Relevance Propagation, Back et al., 2015; 8.Montavon et al., 2017

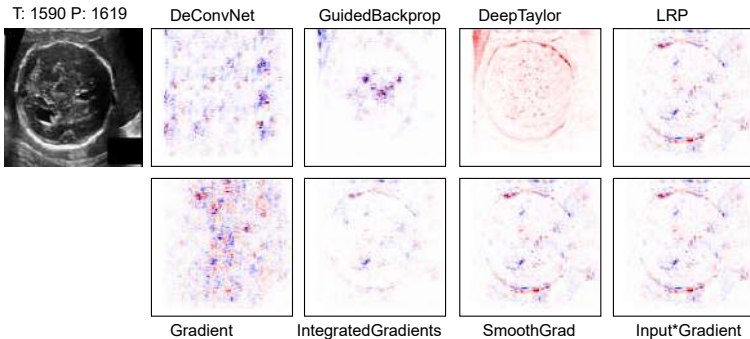
Saliency maps on regression CNN



Saliency maps on regression VGG16

☹ No effective features are retrieved by **DeConvNet** and **Gradient**.
P: predicted HC value, T: ground truth HC value (in pixels).

Saliency maps on regression CNN



Saliency maps on regression ResNet50

☹ DeConvNet and Gradient are insensitive to the models.

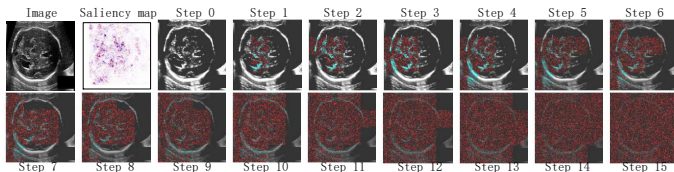
☹ Quantitative criteria is needed.

P: predicted HC value, T: ground truth HC value (in pixels).

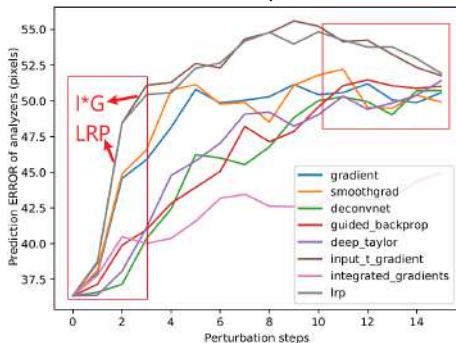
Quantitative evaluation method

Perturbation-based evaluation:

➡ Adding noise according to **importance rank** of saliency map



Perturbation process



Quantitative evaluation method

Area over Perturbation Curve (AOPC) (Samek et al., 2017)

➡ Difference of **accuracy** with/without perturbation in **Classification**

Adapted for **Regression** (Accuracy \rightarrow Error $\epsilon(x_n)$)

$$\text{AOPC}_{\text{Analyzer}}^{\text{regression}} = \frac{1}{N} \sum_{n=0}^N (\epsilon(x_n))^{(0)} - \frac{1}{K} \sum_{k=0}^K \epsilon(x_n)^{(k)} \quad (5)$$

N is the number of images, K is the number of perturbation steps, ϵ is prediction error.

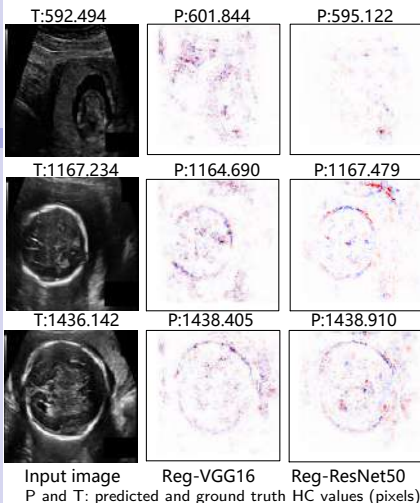
AOPC score:

↑ Models: Sensitive to perturbation

↑ Explanation method: Ability to capture highlight features

Model's explainability Validation

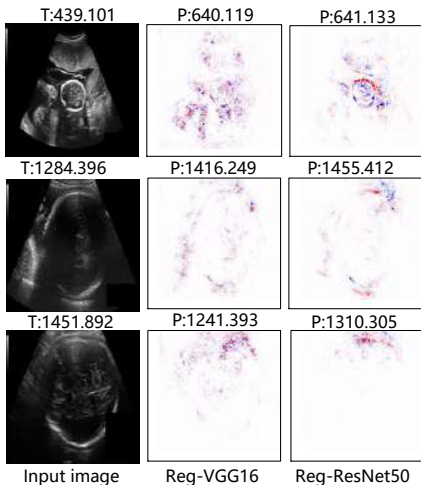
Saliency maps for **good prediction results** on two models



- Input*Gradient method
- Prediction results: **Explainable**
- Reg-ResNet > Reg-VGG

Model's explainability Validation

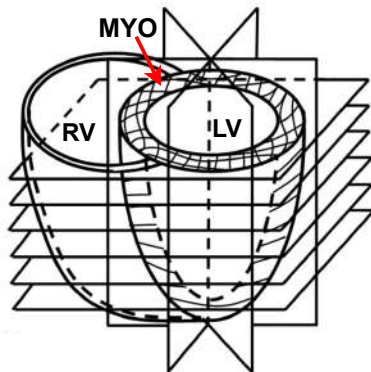
Saliency maps for **bad prediction results** on two models



P and T: predicted and ground truth HC values (pixels).

- Input*Gradient method
- Flaws and biases

Direct cardiac multi-structure volume prediction from 3D MRI images



Cardiac structure

RV: Right Ventricle

MYO: Myocardium

LV: Left Ventricle

ESV: End Systole Volume

EDV: End Diastole Volume

$$\text{Ejection fraction} = \frac{\text{EDV} - \text{ESV}}{\text{EDV}} * 100$$

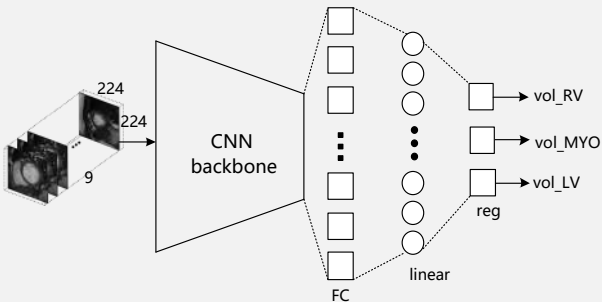
Image credit: <https://doi.org/10.1186/1532-429X-13-36>

Methodology

Goal

Predict the volume of cardiac structures directly **without segmentation**.

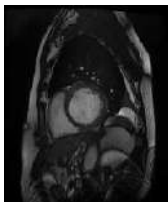
Solution—Regression CNN



ACDC dataset*

Preprocessing

- Slice unifying (9)
- Slice cropping (100*100)
- Data augmentation



P001_fm01



P001_fm01_gt



cropped_P001_fm01

➤ Dataset: 182 subjects

NOR	Train(100)	Valid(32)	Test(50)
MINF			
HCM			
DCM			
RV			

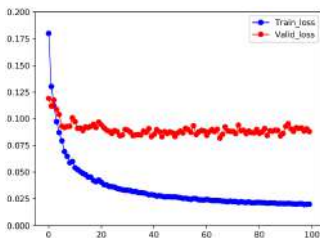
➤ Ground truth: volume of RV, MYO, LV (ml)

$$\text{Volume} = \sum_i^N S_i * px_x * px_y * px_z / 1000 \quad (6)$$

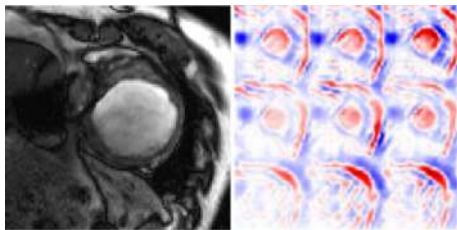
S: Area of cardiac structure; N: Number of cardiac slices; px: pixelsize in x,y,z

* <https://acdc.creatis.insa-lyon.fr/>

Discussion



(a) Loss curve



(b) Saliency map

- Regression CNN model, **over-fitting**
- **Low SNR** in cardiac images.
- The **cardiac slices** may influence the model's prediction

Summary

- ❑ Estimating cardiac structure volume **directly**.
- ❑ Extending **image modality** and **prediction targets**.
- ❑ Experimental results have room for improvement.

Conclusions of thesis

New loss:

- ✓ Kappa loss
- ✓ Generalization of Dice loss
- ✓ Class imbalance & balance problem

Biomarker estimation:

- ✓ Regression CNN—Segmentation-free
- ✓ Head circumference: Seg vs. Seg-free
- ✓ Cardiac structure volume

Model's explainability:

- ✓ Saliency maps on regression CNNs
- ✓ Evaluate explanation methods: Perturbation-based

The end

Thank you for your attention!

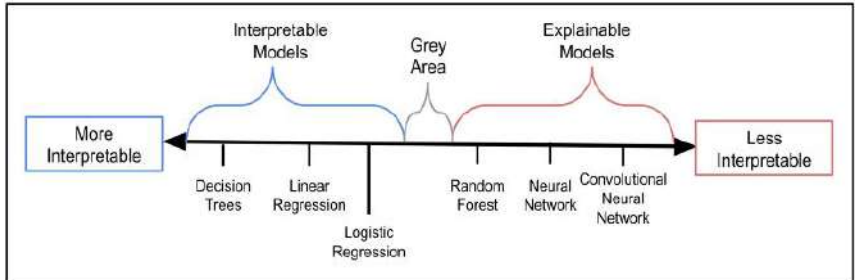
Acknowledgment:

€ China Scholarship Council (CSC)

🖥 Centre Régional Informatique et d'Applications Numériques
de Normandie (CRIANN)



Interpretable and Explainable



Ref: <https://towardsdatascience.com/interperable-vs-explainable-machine-learning-1fa525e12f48>

Additional info

Additional experiments on ACDC dataset:

- The influence of data modality
 - ✔ Cardiac slices
 - ✔ Training data scale
 - ✔ Single cardiac structure vs. Multi-structure
- Hyper parameters
 - ✔ Batchsize and learning rate
 - ✔ Dataset splitting
 - ✔ Data type distribution
- Vision Transformer

Additional info

Active contour loss for segmentation:

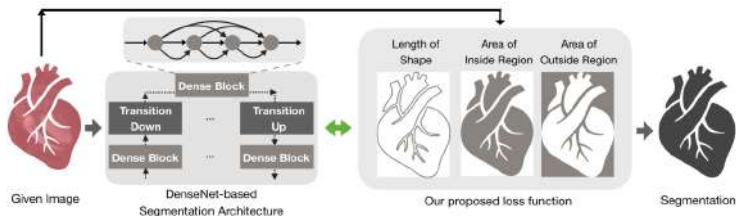


Figure 2: Overview of our proposed method which takes the object's area and length of the boundaries into account during training.

Chen, Xu, et al. "Learning active contour models for medical image segmentation." Proceedings of the IEEE/CVF conference on computer vision and pattern recognition. 2019.

Additional info

Robust loss for regression:

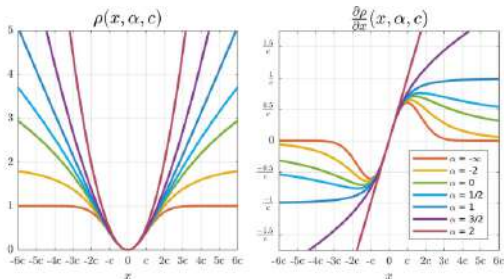


Figure 1. Our general loss function (left) and its gradient (right) for different values of its shape parameter α . Several values of α reproduce existing loss functions: L2 loss ($\alpha = 2$), Charbonnier loss ($\alpha = 1$), Cauchy loss ($\alpha = 0$), Geman-McClure loss ($\alpha = 1/2$), and Welsch loss ($\alpha = -2$), and Welsch loss ($\alpha = -\infty$).

Barron, Jonathan T. "A general and adaptive robust loss function." Proceedings of the IEEE/CVF Conference on Computer Vision and Pattern Recognition. 2019.