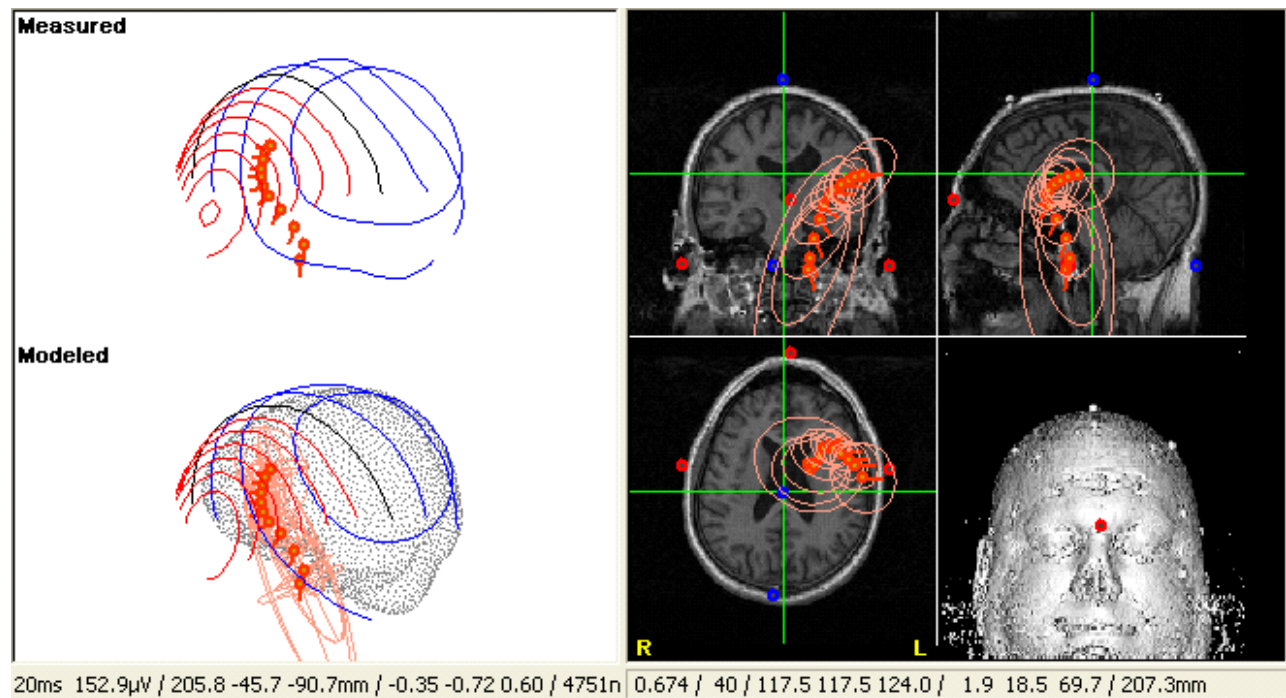


Source V2



Source Reconstruction

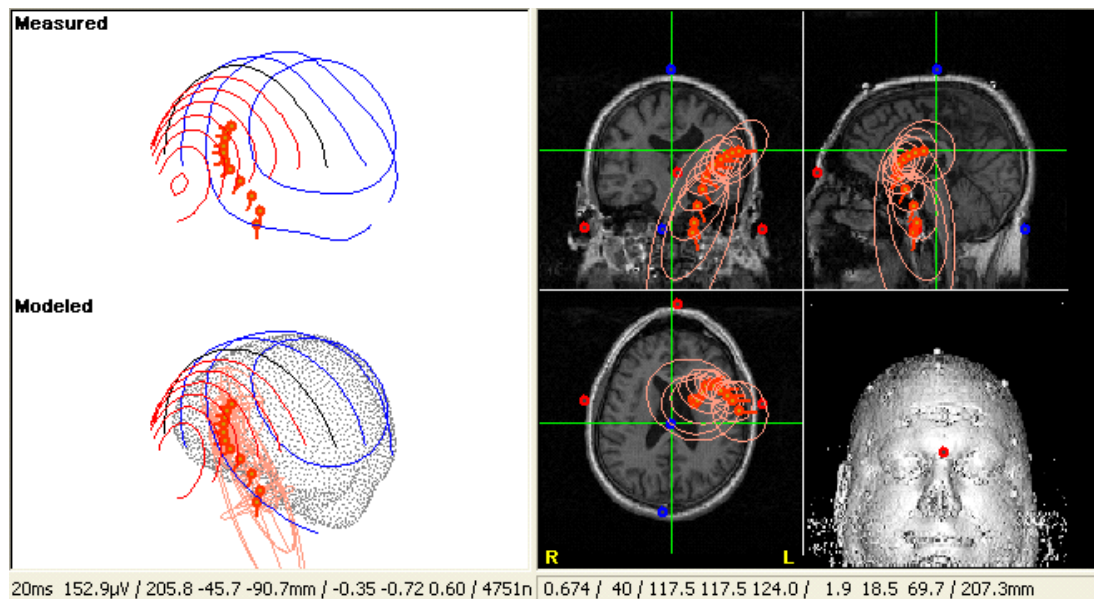


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1 Source V2

SOURCE 2TM *User Manual*



Compumedics USA, Inc.

6605 West W.T. Harris Blvd., Suite F
Charlotte, NC 28269
USA
Telephone: 877-717-3975 (8am - 5pm EST)



Compumedics Germany GmbH
Heussweg 25
20255 Hamburg, Germany
Telephone: +49 40 40 18 99 41
Fax: +49 40 40 18 99 49

Internet: sales@neuroscan.com
techsup@neuroscan.com
www.neuroscan.com



1.1 Contact Information

For Technical Support...

If you have any questions or problems, please contact Technical Support through any of the following routes.

If you live outside the USA or Canada, and purchased your system through one of our international distributors, please contact the **distributor** first, especially if your system is under warranty.

In all other cases, please use **techsup@neuroscan.com**, or see the other Support options on our web site (<http://www.neuroscan.com>).

Or, if you live in the USA or Canada, please call **1-877-717-3975**. International callers should use **1-704-749-3200**.

For Sales related questions, please contact your local distributor, or contact us at **sales@neuroscan.com**.

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7321A SourceV2 45

1.2 The Neuroscan SOURCE Program

The SOURCE™ program runs as part of the ACQUIRE™ and EDIT™ programs in SCAN 4.2™ and newer versions. It provides several models that may be used to calculate one or more dipole solutions for your SCAN averaged, epoched, or continuous data files. Some of the main features include:

- Computation of single equivalent current dipoles, moving dipoles, rotating dipoles, fixed (coh.) dipoles, and fixed (MUSIC) dipoles.
- SOURCE solutions may be calculated online (in ACQUIRE) or off-line (in EDIT).
- The results are displayed on skin, skull, and/or brain point clouds, or on a generic MRI head display (or you may import your own MRI/CT data).
- An equivalent electrode label matching algorithm recognizes and includes variations on the 10-20 system labels, or you may import your own electrode position information.
- Dipoles are calculated using a three concentric spheres model, a standard or interpolated Boundary Element Model (BEM), or an interpolated Finite Element Model (FEM).
- Single point or user-defined latency interval analyses.
- Displays of measured and fitted contours.
- Confidence ellipsoids for dipole solutions.
- Easy methods for viewing the results from various perspectives, and options for displaying skin, skull and brain point clouds.
- Default or user-determined radii and conductivities.
- Manual repositioning of the dipole source for hypothesis testing.

The programs are easily installed and quickly mastered. If you have any questions or difficulties, please contact Technical Support (see above).

1.3 Installing SOURCE

SOURCE and its related files are installed automatically from the SCAN 4.5 CD (or newer version). The actual programs used are SourceOCX.ocx, SliceOCX.ocx, a compatible version of acquire.exe, and some ancillary files. These will be copied to your Scan4.5 folder, along with some demonstration files.

2 Quick Introduction to SOURCE

The following is a step by step tutorial designed to introduce you to the operation and many of the capabilities of SOURCE. The details for all of the options and parameter settings are found in the later sections. The general steps that you will perform in routine

use are:

- Load the Data Files
- Perform PCA and ICA Decomposition
- Perform Source Reconstruction
- Display the Results
- Importing Your Own Image Data (if available)



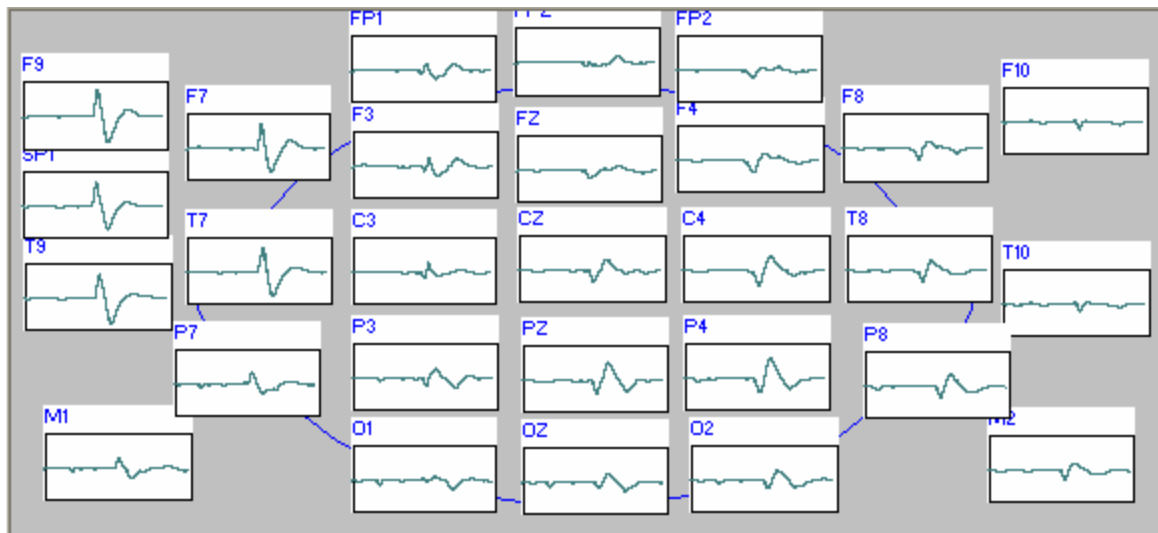
Note

If you apply transforms in EDIT to the same data file that is being used in SOURCE, the transforms will NOT be transferred to the file in SOURCE.

Load the Data Files. The first steps in using SOURCE (offline) involve selecting the data file you want to use and the electrode position file that goes with it, if available. If you have the Image Data file (CT or MRI), you can retrieve that file in a later step.



1 Retrieve the data file in EDIT, as usual. This can be an .avg, .eeg, or .cnt file. The *EpiSpike.avg* file was selected below (from the ...\\Scan Data\\Demo File\\EEG Spikes folder).




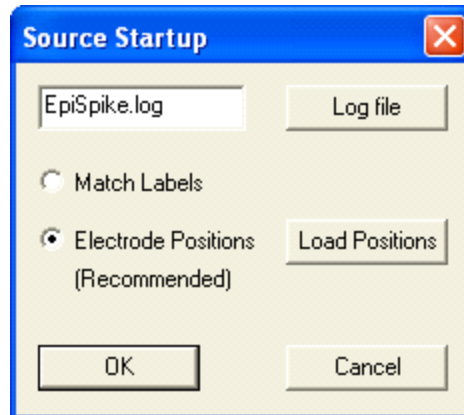
2 The next step depends on whether you have the .3dd file from 3DSpaceDx. This is a file, created with a digitizer device, which contains the 3D locations of the electrodes and the functional landmarks (nasion, left preauricular, and right preauricular, at least). If you do not have this file, then you can still use SOURCE as long as you have conventional names for the electrodes.

If you do have the file, you have two options. You can *right click* between electrode displays and use **Load 3D Electrode positions** to select and merge the .3dd file with the data file. Or, you can start SOURCE and select the file in the first screen. We will demonstrate the second option here.

3 It is necessary to enlarge one electrode window in order to define the Timerange for analysis (or select the single time point for analysis). Enlarge, for example, the T7

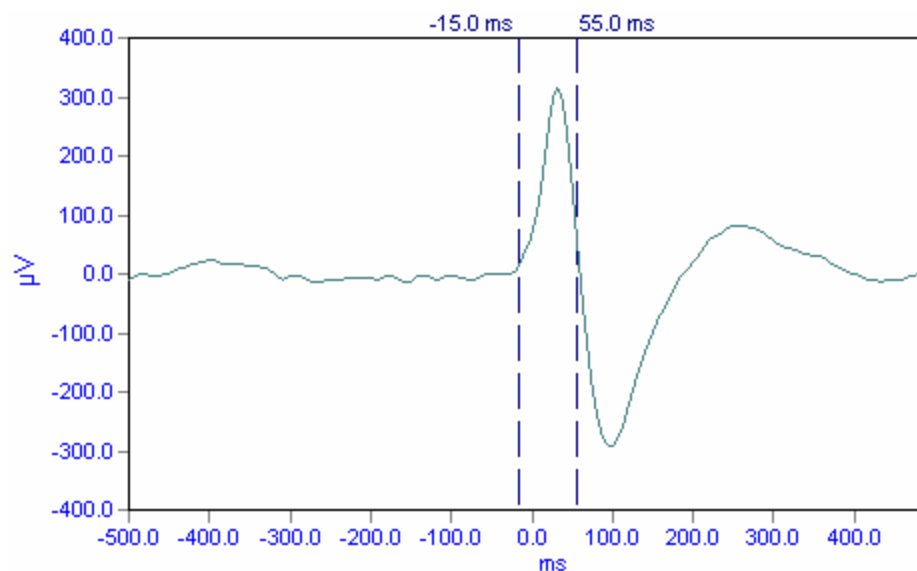
window to at least mid-size.

4 Click the SOURCE icon  to start the program. The Source Startup screen appears. We will use the .log file, as displayed. If we did not have the .3dd file, we would select the **Match Labels** option. Since we do have it, select **Electrode Positions** and click the **Load Positions** button. Select the *EpiSpike.3dd* file and click **OK**.



5 You should then see the SOURCE program open.

6 Looking at the waveforms, you will see one or two dashed vertical lines. There are two modes for using SOURCE - Tracking Mode and Interval Mode. Tracking Mode lets you analyze single time points; Interval Mode lets you analyze all the points within a defined Timerange. *Right click* in the display and select **Use Interval Mode for Source**, if needed. If you still see one dashed vertical line, there are really two lines, one on top of the other. Use the mouse to drag the lines to create the interval between approximately -15 to 55ms. This is the spike part of the waveform. We are selecting that interval to perform source reconstruction in the earliest part of the complex.

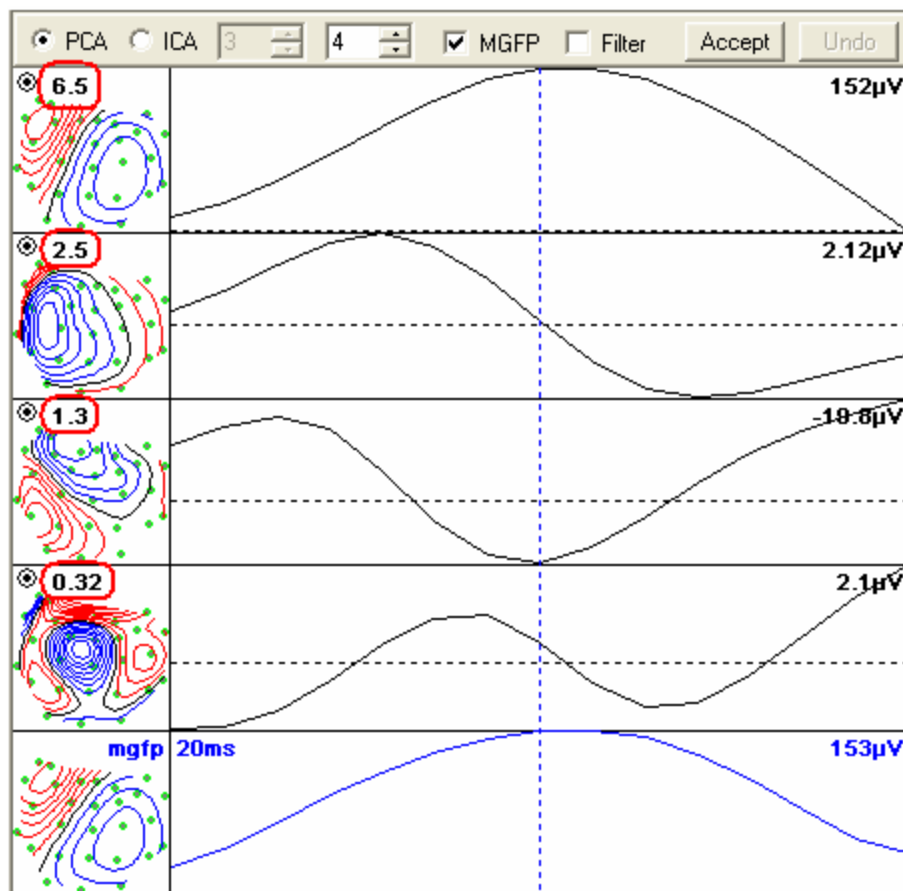


Perform PCA and ICA Decomposition. Principle and Independent Component Analyses may be used to decompose the selected Timerange into components. If there are multiple independent components in the Timerange, there may be multiple sources for each of them. PCA and ICA details are presented in Appendix D following the EDIT manual. In practice, PCA is typically used to determine the number of valid components, and then ICA is used to include or exclude the components in source analyses.



1 Click the PCA\ICA icon from the Toolbar . The PCA\ICA window will appear.

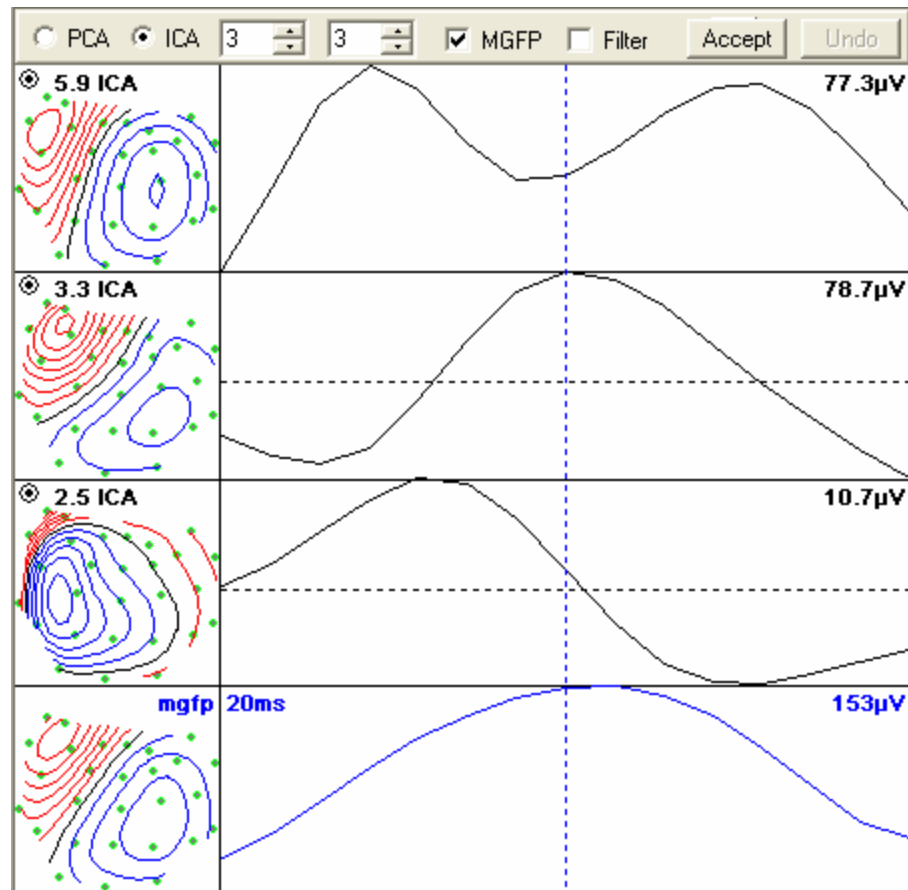
2 Select ☒ PCA, increase the number of displayed components to , and enable ☒ MGFP (Mean Global Field Power - a variability measure across channels). The Timerange selected above (-15 to 55ms) has been decomposed into 4 components, or loadings. The distribution for each loading is displayed on the left (contour maps). Above each map is the SNR value (Signal to Noise Ratio). If you see percentages instead, right click in the display and select **Show SNR values**.



For a component to be considered valid, the SNR value should be *greater than 1.0*. The first three components are valid, while the fourth is not.

3 Select **ICA** and set the number of computed and displayed components to **3**

ICA 3 3. This means that within the Timerange we selected (-15 to 55ms), there are 3 independent components. The distributions for each are shown in the contour maps.



With ICA, you have the ability to include or exclude any of the components. If one of the components were clearly artifactual in origin (such as an eye blink artifact), we could exclude that component from source reconstruction. Looking at the distributions of these three components, none appears to be artifactual in origin. We decide therefore to leave all three components in.

Perform Source Reconstruction. The next step is to select the dipole model and volume conductor to use. *Right click* in the SOURCE display, and select **Source Parameters**.



1 First, we need to decide which Dipole model to use. In this case, we know from experience and from the literature that a Moving dipole is the better model to use when investigating the sources of epileptic spike activity. Select **Moving**.

dipole model

☒ moving
 ☐ rotating
 ☐ regional
 ☐ fixed (coh.)
 ☐ fixed (MUSIC)

number of dipoles:
 min. distance [mm]:
 seed distance [mm]:

threshold [%]:
☐ mirrored (xy-plane)

noise level [μ V]:
☐ add test-dipole

With a moving dipole, there is one dipole for each time point in the Timerange. If we were using a different model, we might want to increase the number of dipoles, since there are three ICA components in the Timerange. Leave the **Minimum Distance** between solutions at **10mm**, and the **Seed Distance** at **200mm** (large enough to include the entire head). Set the **Threshold** at **70%**. The noise level has been computed automatically. You can enter a different value under special circumstances where you want to test different noise levels. Generally, you should not change the computed noise level.

2 Next, we need to decide which Volume Conductor to use. The BEM and FEM volume conductors have been created already from the Montreal Neurological Institute (MNI) averaged MR data set. (Unlike CURRY, you cannot create a BEM model from the individual's MR data using SOURCE). Generally, any of them will be more accurate than the 3 Spherical Shells models, although, depending on where the source is, there may be little difference. The differences among the BEM and FEM models are usually very slight.

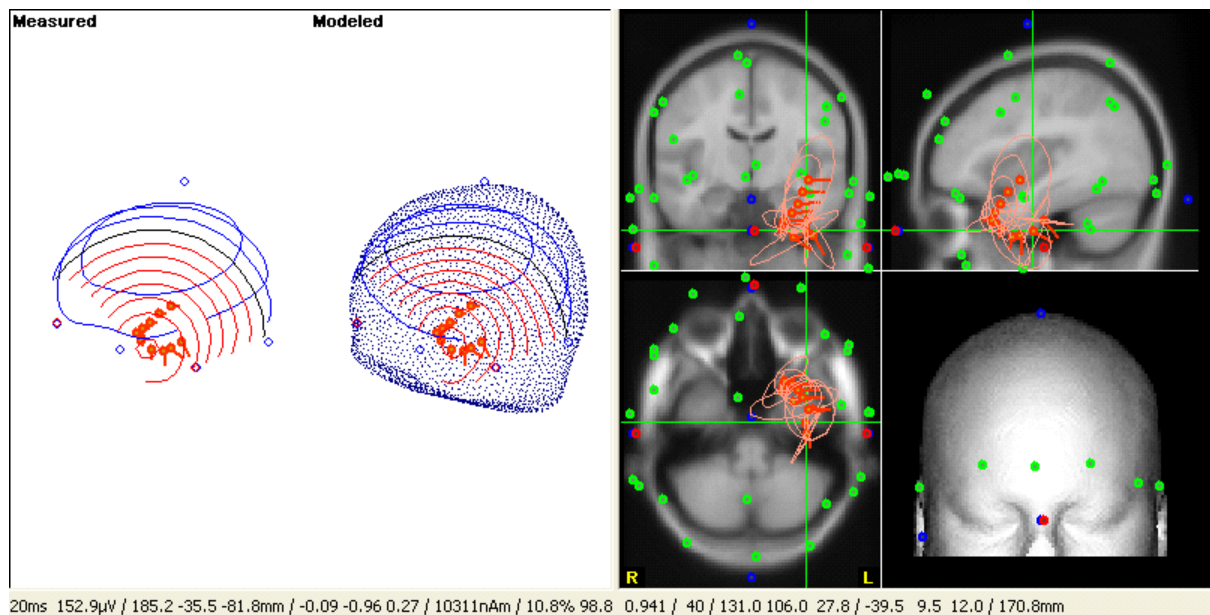
volume conductor model

☐ three spherical shells
 ☒ standard BEM
 ☐ BEM interpolated
 ☐ FEM interpolated

relative radii [%]:

conductivities [S/m]:

In this case, where the sources are in the temporal lobe, any of the BEM or FEM models will be more accurate than the 3 Spherical Shells models. Select the **Standard BEM** model, and click **Apply**.



Display the Results. The dipole solutions are shown in the SOURCE and SLICE displays. What you see displayed is determined from the context menus in both screens.



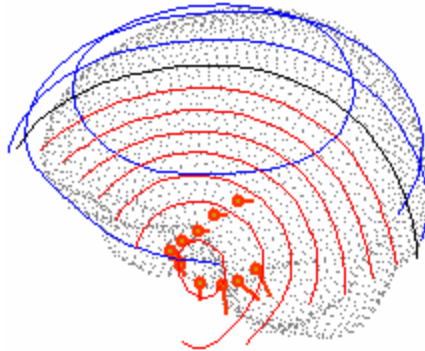
1 Right click in the SOURCE display and select **View** → **Left View** (or *Alt+L*), if needed. You can see that the dipole solutions trace around the tip of the left temporal lobe.

2 You can display any combination of the Skin, Skull, or Brain point clouds, as well as other objects. Right click in the SOURCE display as needed to select only the **Contour Lines** and **Brain** point cloud. Note that there are *keyboard* controls for these.

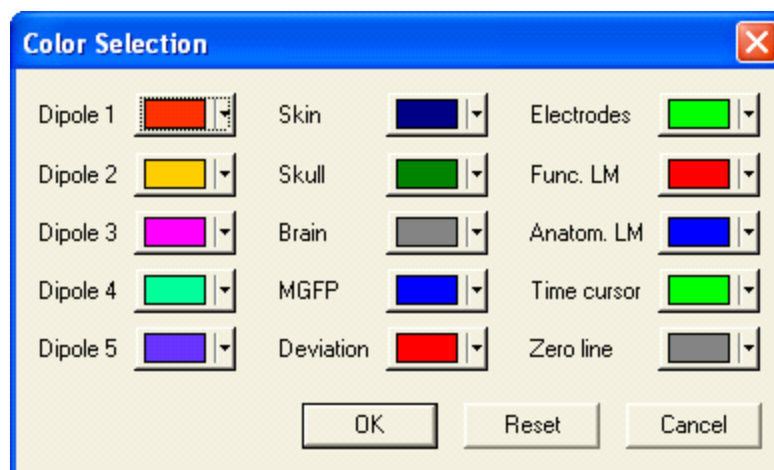
<input checked="" type="checkbox"/>	Contour Lines	C
<input type="checkbox"/>	Electrodes	E
<input type="checkbox"/>	Landmarks	L
<input type="checkbox"/>	Volume Conductor	V
<input type="checkbox"/>	Skin	Alt+S
<input type="checkbox"/>	Skull	Alt+K
<input checked="" type="checkbox"/>	Brain	Alt+B

Note that you can grab and drag the image to different views. Use the *mouse wheel* to increase or decrease the size (or hold the *right mouse* button down and move the cursor up and down). Right click in the display and select **Movie** (*M*) to see a progression of the solutions for each data point in the Timerange. To change the speed of the Movie display, increase or decrease the **movie/rotation delay (ms)** parameter (in the Source Parameters screen). You can rotate the image by *right clicking* and selecting **Rotation (360 degrees)**. The speed of the rotation is also controlled by the **movie/rotation delay** parameter. Movies and Rotations may be

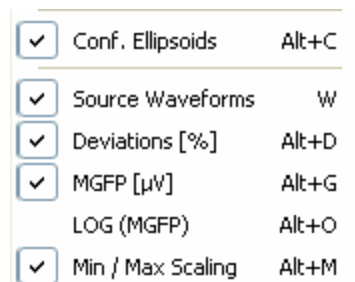
saved as AVI movies (*right click* and select one of the Save options). The spacing for the contour lines is controlled by the **contour increment (μV)** parameter (in the Source Parameters screen).



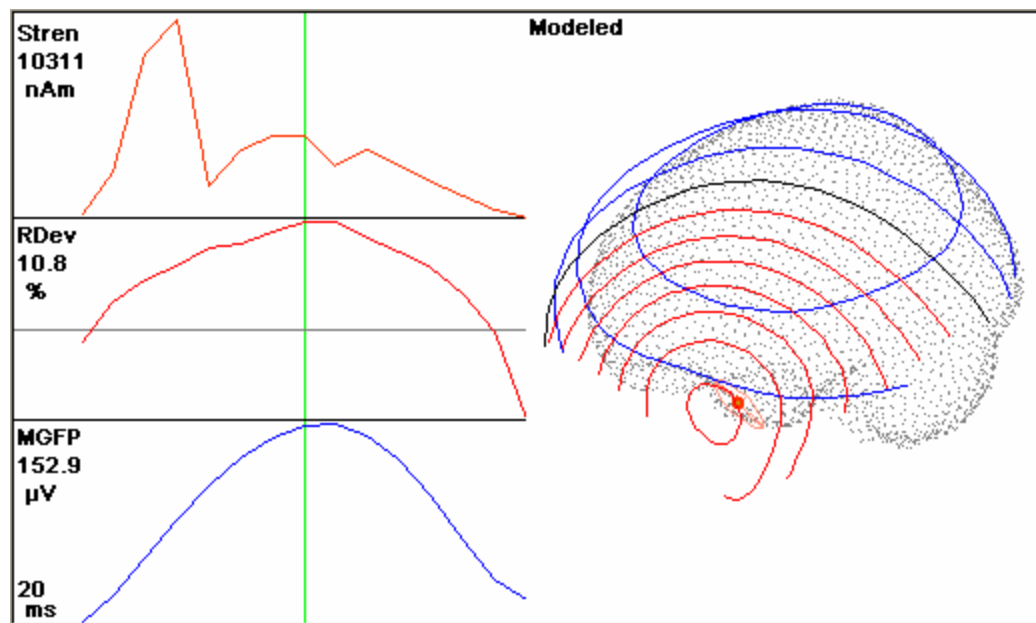
3 *Right click* in the SOURCE display and select **Colors**. You can then set different colors for various parts of the display. Click **Reset** to restore the default colors.



4 *Right click* again in the SOURCE display and select **Display** → **Source Waveforms**, then *right click* again and select **Display** → **Confidence Ellipsoids**.

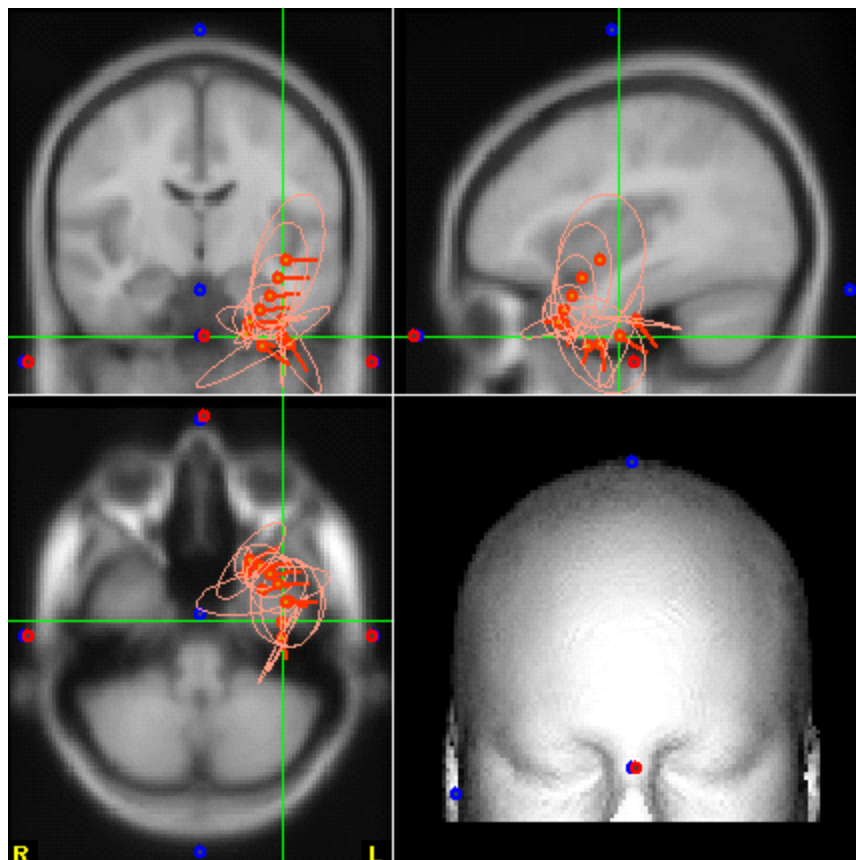


Now when you move the middle cursor, you can see the progression of the dipoles across time. Notice that the confidence ellipsoids (the 95% confidence area) for each dipole solution change in size. Obviously, the smaller the ellipsoid, the better the solution.



Right click in the display and deselect **Display** → **Source Waveforms**. (This is necessary to see all of the solutions in the next step).

5 You can also see the dipoles on the MR data in the SLICE display. If you do not see the dipoles, *right click* and select **Display** → **Dipoles**.



Grab the crosshair in one of the views and move it around to see the corresponding changes in the other views.

In this case the averaged MR data are displayed. As with the SOURCE display, the display options are accessed from the context menu. *Right click* in the display and select different **Display** and **View** options.

Next, we will import the subject's MR data.

Importing Your Own Image Data.

If you have MR data for the subject, you can import it into SOURCE and display the dipole solutions on the individual's own brain images. Unlike CURRY, however, you cannot compute a realistic volume conductor model using the individual's MR data. You can coregister the two data sets using the functional and anatomical landmarks.



1 *Right click* in the SLICE display and click **Select Data**. Retrieve the *MRI.img* file. In this case, the image data parameter file already exists (.imp extension). If you were retrieving the file for the first time you would need to verify/supply the parameters.

2 *Right click* in the SLICE display and select **Data Parameters**.

SLICE: Image Parameters

Image Data Parameters

Bits per Pixel: ☐ 8 ☐ 12 ☒ 16 Significant Bits:

Swap Bytes: ☐ Intensity [%]: Header Size [Bytes]:

No. of Pixels: Horizontal Vertical No. of Slices:

Pixelsize [mm]: Horizontal Vertical Distance [mm]:

Slice Orientation / Order

☐ Sagittal ☒ Axial ☐ Coronal ☐ Iso

☐ Invert X (Right - Left) ☒ Invert Y (Front - Back) ☐ Invert Z (Bottom - Up)

Anatomical Landmarks [mm]

Nasion: Vertex:

LPA: Inion:

RPA:

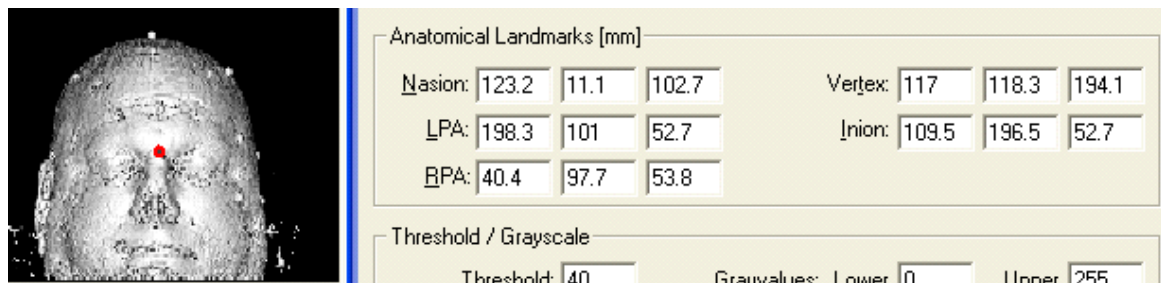
Threshold / Grayscale

Threshold: Grayvalues: Lower Upper

The Image Data Parameters and Slice Orientation/Order sections contain the parameters that must be known about the MR data file in order to load it. SOURCE will attempt to autodetect as many parameters as possible from the data file header, but the information is not always there, and not always accurate. You will need to verify all of the fields based on your particular scanner's settings. You would then click **Apply** to see the image data.

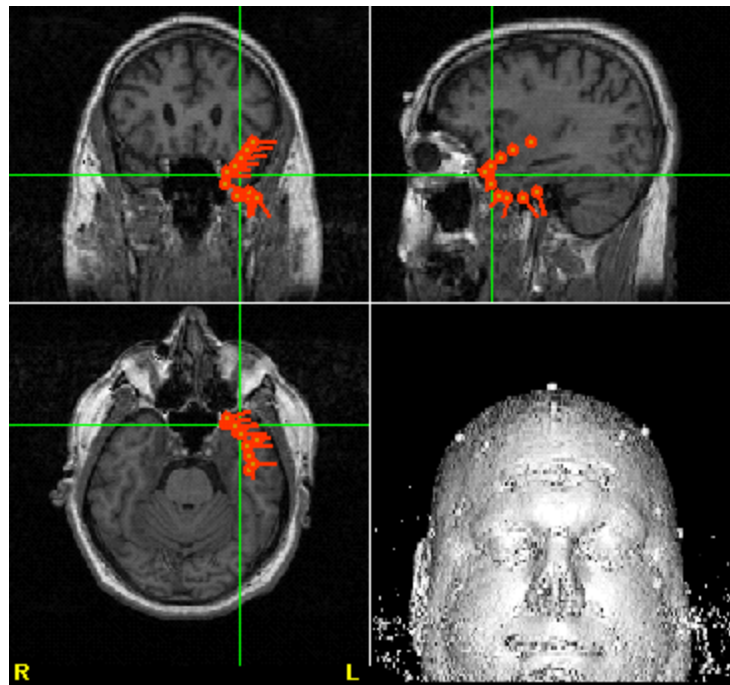
You may need to adjust the **Slice Parameters**, **Threshold** and **Grayscale** levels as well (click the **Apply** button to see the effects).

3 Lastly, you must determine the anatomical landmarks. If these are not entered, or not entered correctly, you will not be able to display the dipole solutions on the MR data. The basic process is as follows.



Position the mouse at the nasion on the rendered view (lower right corner) in the Image Data display. Then *right click* and select **Set Nasion** (*Ctrl+N*). The values will be transferred to the Anatomical Landmarks fields. Then change the rendered view to whatever view is needed for the next landmark (e.g., Left View). Click the left mouse button on the preauricular point, then click the *right mouse* button and select **Set LPA** (*Ctrl+L*). Continue the process until all five landmarks have been measured, then click the **Apply** button. This creates a new .ips file that contains the parameters. The next time you load the image data file, the information will be read from the .ips file, and you will not have to enter it again. With the landmarks correctly identified, you will be able to display the dipole results on the MR images. The landmarks are not, however, used in BEM models, as SOURCE uses the MNI averaged data set only.

When you have imported the MR data and defined the anatomical landmarks, you will see the dipole results displayed on the subject's own MR data. The realistic BEM model and the individual MR data provide the most accurate solutions.



This concludes the basic SOURCE Tutorial. Further examples using SOURCE are presented next, along with some of the rationales for the analysis decisions that were made. Complete details of all of the options in SOURCE are presented after the examples.

3 Some tips for using SOURCE

Users new to source reconstruction techniques typically ask questions like: Which dipole model do I use with my data? How do I know what options to use, and what settings to select? How do I interpret the results from the Source Waveform, Deviations, and MGFP?

Which volume conductor model should I use? At this point in time, there are no absolute answers to many of these kinds of questions. Source reconstruction is a hypothesis driven analysis. Therefore, the approach adopted for source reconstruction must be driven by *a priori* assumptions and by known physiological constraints. Even then, it may not be possible to decide which reconstruction model to apply. If you are not sure which dipole or volume conductor model to use, try several different ones. Look for converging results across models. Look for results that are reasonable. Use common sense, and rely on established neuroanatomy and neurophysiology as much as possible. For example, if you are looking at dipole source solutions for the major components of an SEP recording, it may not make sense to look for multiple dipoles with mirrored results. With auditory stimuli, it is reasonable to expect bilateral, homologous dipoles. In other instances, the expectations and predictions may be more ambiguous. Let's go through a couple of examples, and include some of the thought processes.

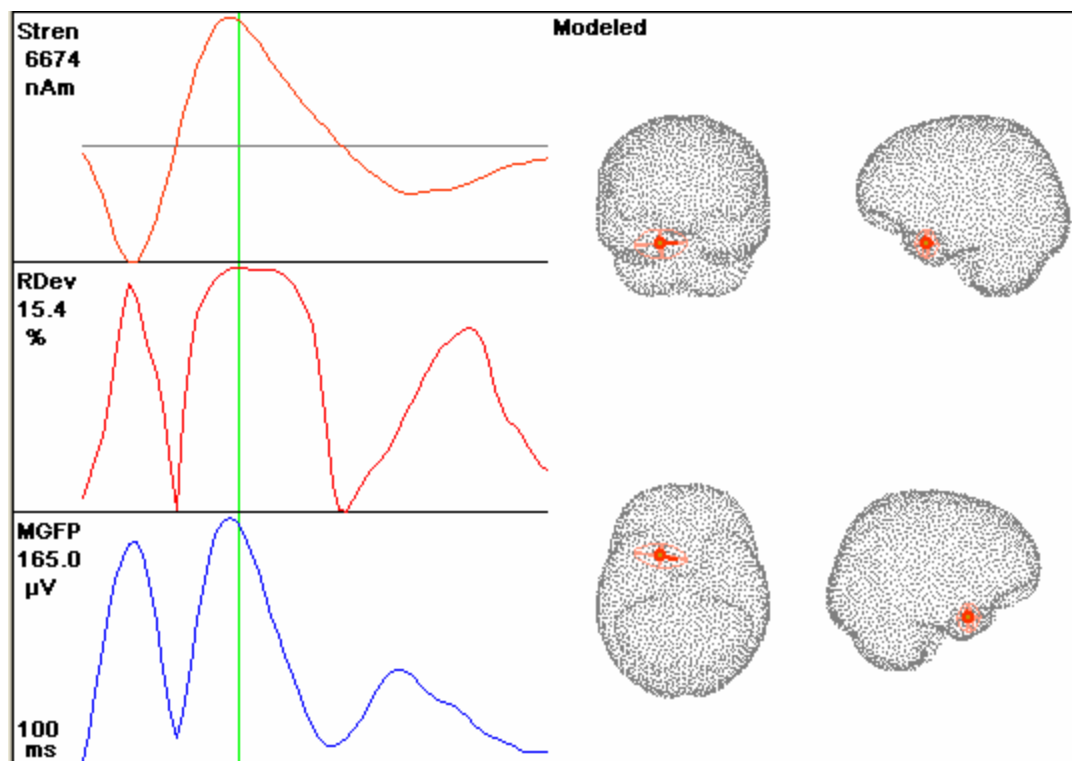
SOURCE and PCA/ICA

Neuroscan provides Principle and Independent Component Analysis (PCA and ICA) options that can be very useful with source reconstruction. After selecting a Timerange for reconstruction, you can then decompose the interval into its components. With ICA, you can select independent components to retain in or remove from the interval. Reconstruction is then computed using the "filtered" waveforms. Please see Appendix D at the end of the EDIT manual for details regarding PCA/ICA, and examples for their use with SOURCE.

3.1 Example 1

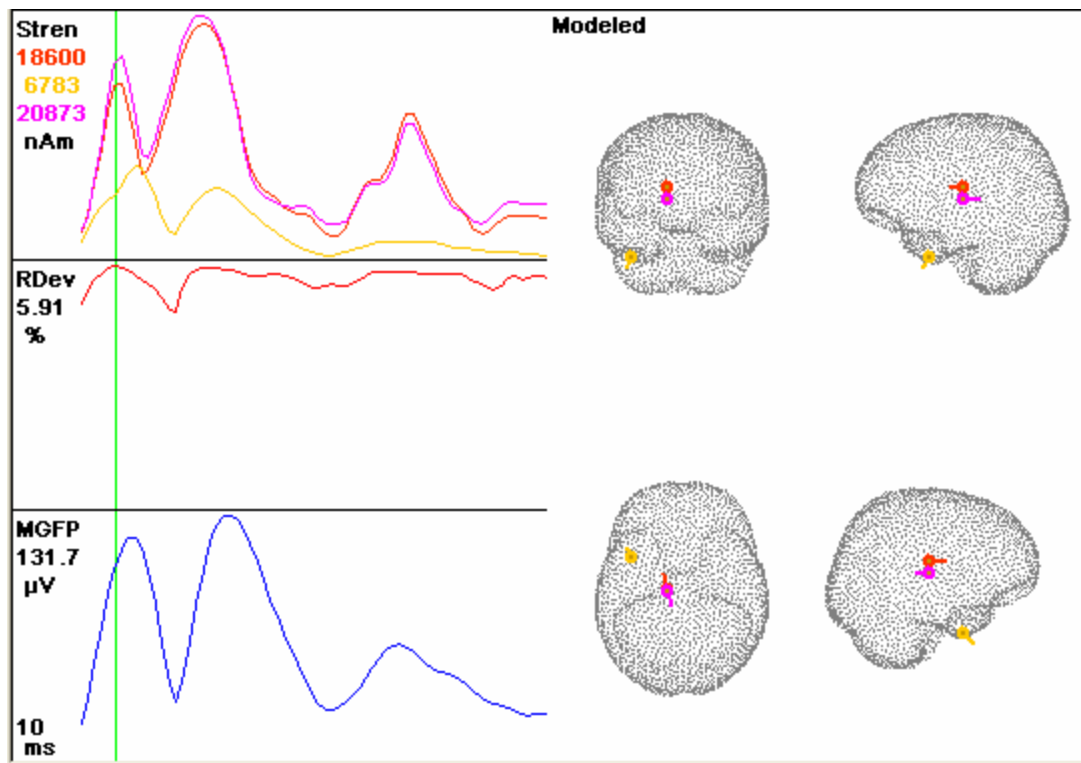
Retrieve the *EpiSpike.avg* demo file, and load the electrodes positions using the *EpiSpike.3dd* file (you should use the actual measured positions whenever possible). This is a single sweep of EEG showing an epileptic spike and slow wave complex from the left frontotemporal region. The question we might ask is, what is the anatomical source of the spike? Even if prior studies have shown some consistencies for localization of epileptic spikes, it may be that there is insufficient information to make an *a priori* decision as to which reconstruction method we should use. (In fact, our prior experience indicates that a moving dipole is the best model to use in these instances, but, for the sake of demonstration, let us assume we have no prior knowledge).

Select the interval between about -15 and 330ms to encompass the entire spike and slow wave interval. For demonstration's sake, we will apply the Fixed (MUSIC) model (single dipole) and the BEM interpolated volume conductor model, which should give good results for temporally independent sources with fixed orientations.



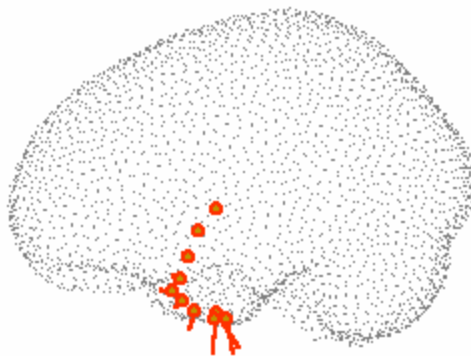
Over the entire interval, we see a localization in the left medial frontotemporal lobe area. Now look at the MGFP and Deviations results. The MGFP is an averaged measure for the signal strength (and thus the Signal to Noise Ratio, or SNR). One can easily distinguish latency ranges with meaningful signal from noise or background activity periods. Estimating the SNR from the MGFP together with the Deviations percentage can tell you if the chosen source model is at least able to explain the signal part of your data. For example, assume an SNR of 10 ($10\mu\text{V}$ signal / $1\mu\text{V}$ noise), then an adequate source model should be able to explain the signal part resulting in a residual deviation of about 10%. If one has a better fit with less than 10% deviation, one starts to fit the noise (e.g. when taking too many dipoles resulting in meaningless dipole positions, but with well explained data). On the other hand, when the fit quality (deviation) is on the order of 20% (which would correspond to an SNR of 5) only, the source model is not adequate (or the SNR was not estimated very well). Keeping in mind that an adequate source model should exhibit similar traces for MGFP and explained deviation (at latencies with high MGFP and thus high SNR, the explained deviation should be high, and the residual deviation, which equals $1 - \text{explained deviation}$, should be low).

Note that there appear to be at least 2 dipoles in the analysis interval (if we use PCA and ICA analyses, we would find that there are 3 valid components in this interval). We may want to run the analyses using the suggested intervals. First, however, for interest's sake, we decide to use the Rotating dipole model (this time with 3 dipoles).



Again we see dipole solutions in the left temporal area. Use the M key to play the Movie of the results, or use the arrow keys to step through the analysis interval one point at a time. The solutions show an interesting rotation during the interval.

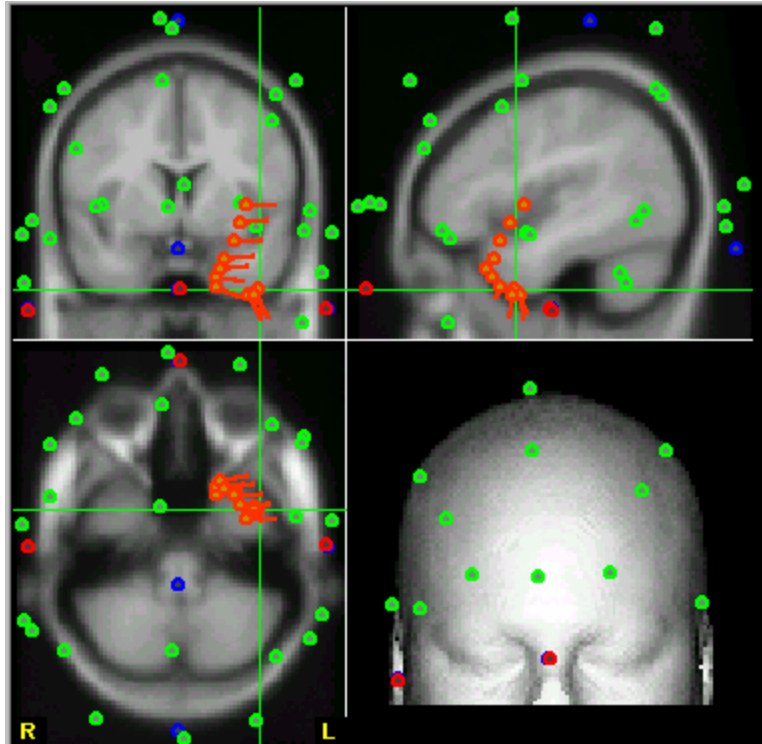
We then decide to use the Moving dipole model, and limit the interval to the 0-50ms span (based on the first peak in the MGFP, Deviations, and signal strength). Disable the Source Waveforms option to see the results. Increased the threshold to 75% to display only the most robust solutions.



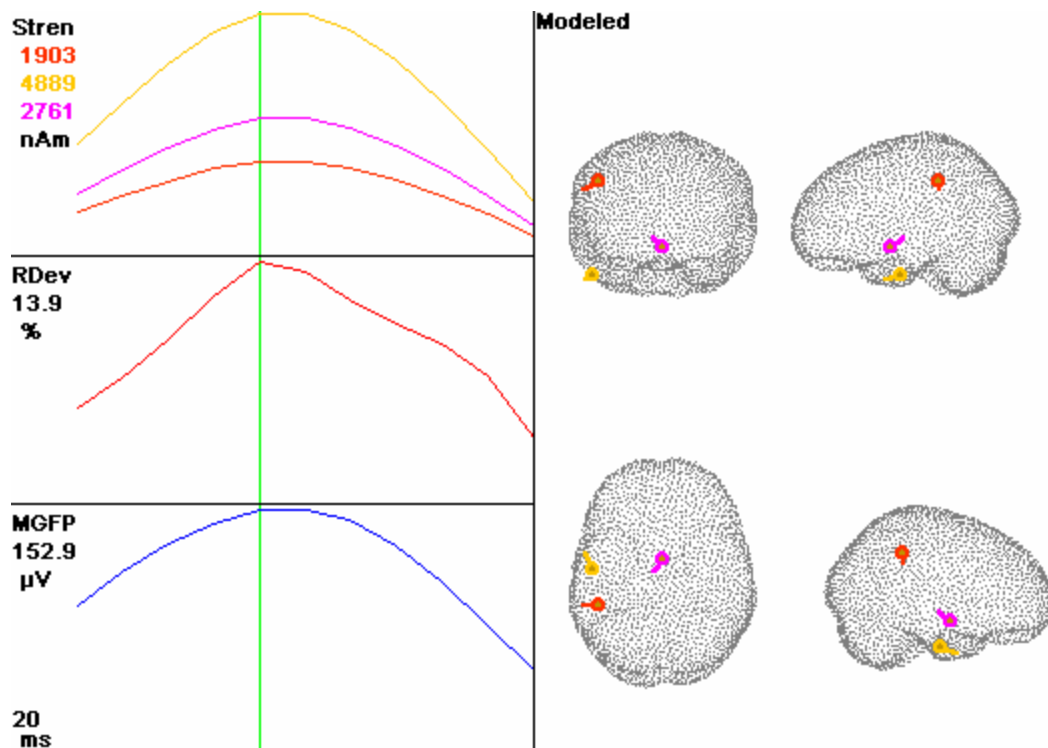
Now we see an interesting progression through the analysis interval. Play the movie now, and see the progression from inferior to relatively superior sites, following the contour of the anterior tip of the left temporal lobe. The SLICE display also points to the general anterior temporal lobe area. (Note that left and right are reversed on the SLICE display).

If we compare these results to those of the prior analysis methods, we see a correlation

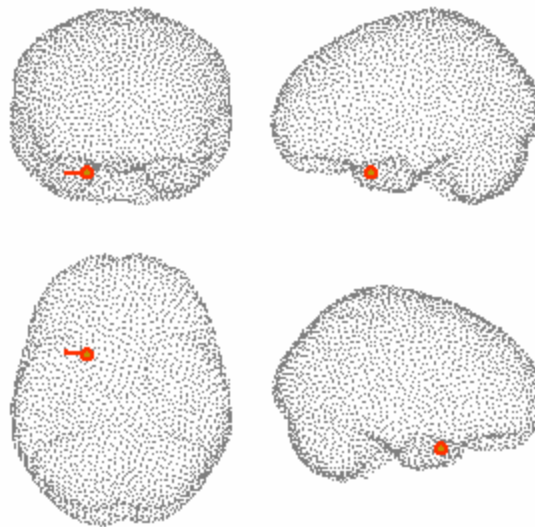
among the dipole sources. For example, looking at the 3 points resulting from the Rotating dipole analyses, we see that those 3 solutions fall nearly on the same line as shown above. The single dipole solution we began with falls more or less in the middle of the path of the moving dipole. In general, the above methods provide converging validation for the left anterior temporal lobe (apparently a progression along the anterior tip of the lobe) as the source of this spike.



For comparison's sake, we decided to look at the Fixed (coh) method, solving for 3 dipoles, during the 0-50ms span.



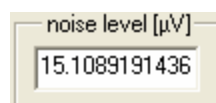
We see first of all that one solution is in the centroparietal area, and another is nearly on the midline. This suggests that this model may not be appropriate. Rerunning the analysis with a single dipole gives the approximate left medial frontotemporal lobe location.



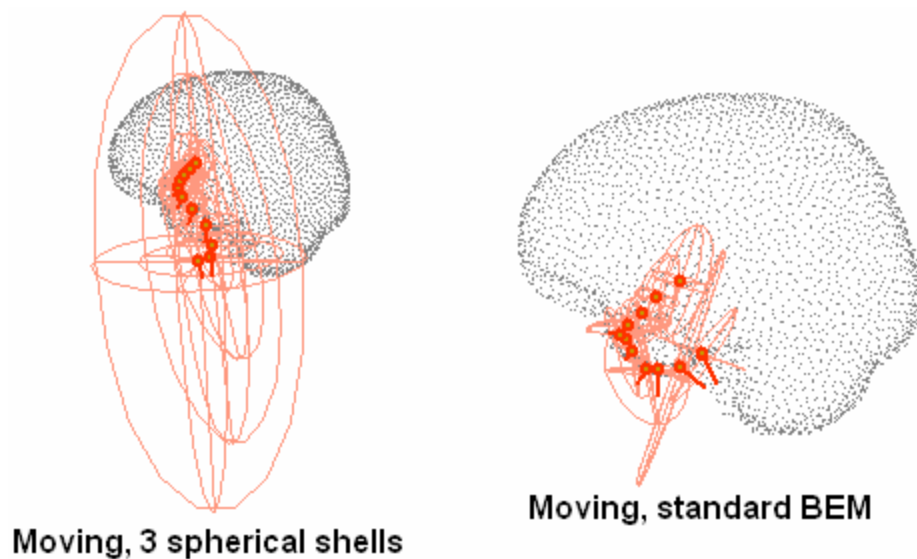
Keep in mind that source reconstruction is somewhat of an art, and there are frequently no straightforward procedures to follow. You typically have to try several source models and volume conductor models until you meet your expectations of the underlying brain activity (based on your *a priori* assumptions), and until the chosen models can explain your data. The inverse problem has no unique solution! Only with additional assumptions like the number and characteristics (moving, rotating, fixed, coherent) of the sources can a unique solution (in a mathematical sense) be achieved. For example, three fixed dipoles

can explain well enough the spike of the spike wave complex we analyzed above, and three rotating sources can explain the data even better since they have more degrees of freedom. However, the "true" source model would be a moving dipole in this case - from the residual deviation alone you cannot judge for or against one model - you have to know about the physiological aspects to find the adequate model. Also, different volume conductor models lead to different dipole localizations, but both models may be able to explain the measured data.

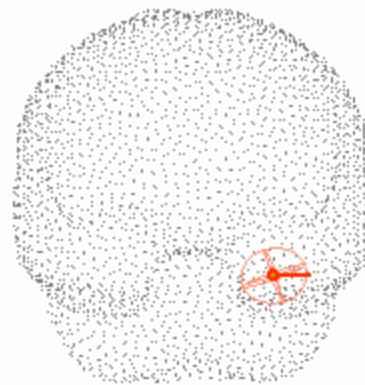
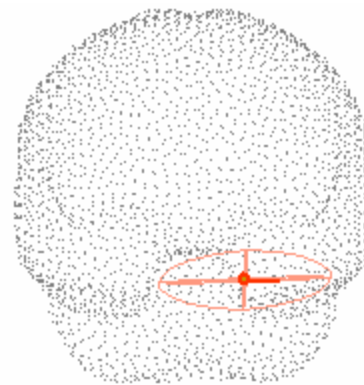
The Confidence Intervals, or ellipsoids, give additional information that is useful for determining the best dipole and volume conductor models to use. The axes of the ellipsoids are proportional to the estimated noise level. The noise level is estimated by analyzing the MGFP in the prestimulus interval, and that value is entered automatically in the Source Parameters dialog box.



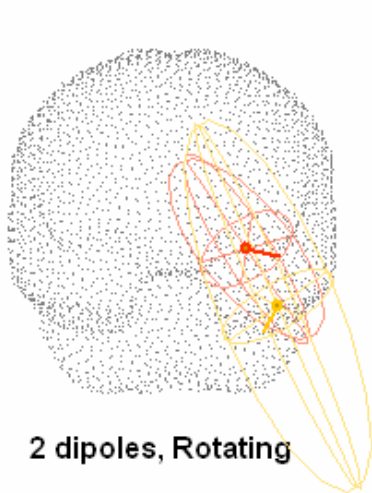
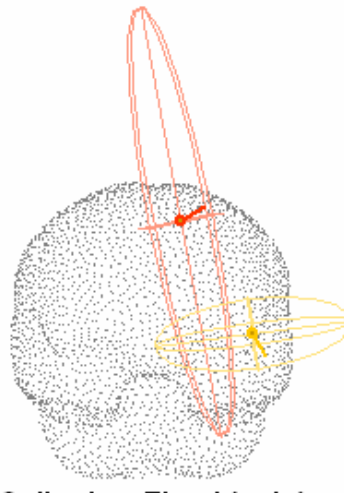
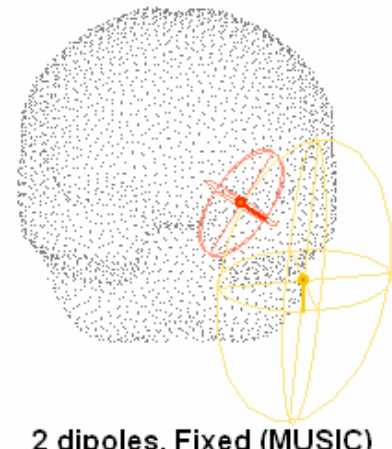
Select the time range from -15 to 55ms, with a threshold of 75%. By trying different dipole models, and different volume conductor models, you can see which combination produces the smallest confidence ellipsoids. For example, the confidence intervals are smaller when using the standard BEM volume conductor with a moving dipole model, than with the three spherical shells model. (Rotate the display to see the ellipsoids from all angles).



In the example below, the rotating dipole model gives a smaller confidence ellipsoid than the fixed (MUSIC) model.

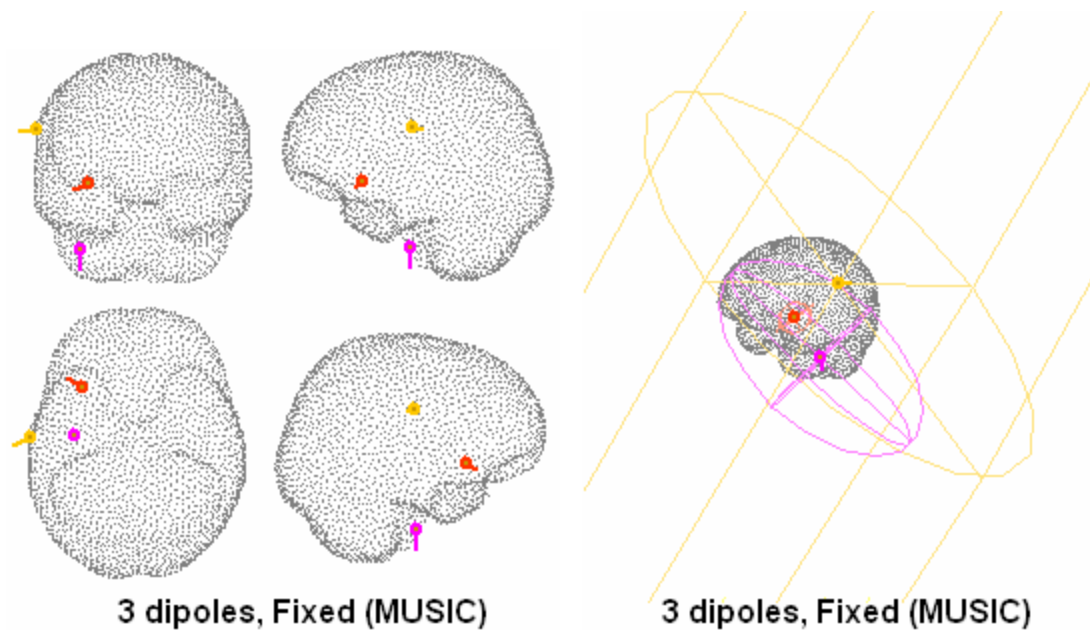
**Rotating dipole model****Fixed (MUSIC) model**

The confidence ellipsoids are also helpful in deciding whether multiple dipole sources are appropriate. In this example, we solved for 2 dipoles (using a three spherical shell model).

**2 dipoles, Rotating****2 dipoles, Fixed (coh.)****2 dipoles, Fixed (MUSIC)**

None of the models looks particularly valid since the ellipsoids are rather large. The Fixed (MUSIC) and the Rotating models are perhaps preferable to the Fixed (coh.) model (where the position of one solution is in the wrong area).

Solving for 3 dipoles might seem like a reasonable thing to do, until you look at the confidence ellipsoids:

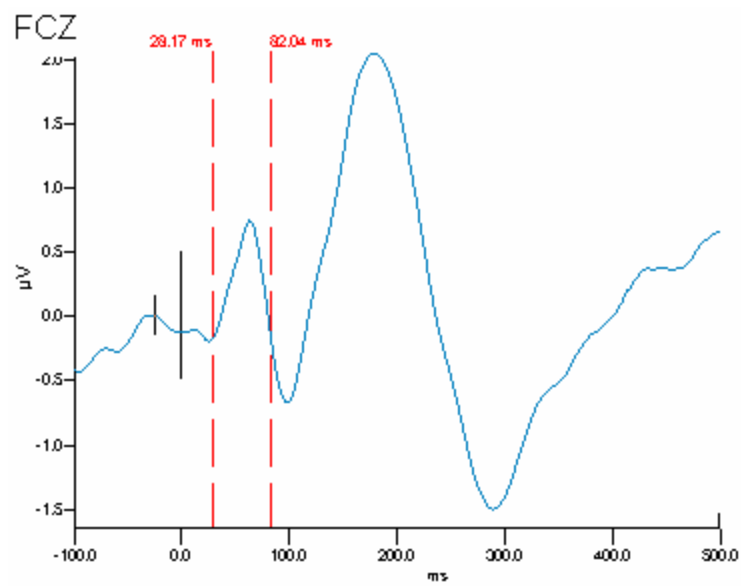


The extreme range of the ellipsoids clearly indicates that this is a bad model. Without the confidence ellipsoids, one might be tempted to accept the 3 dipole locations.

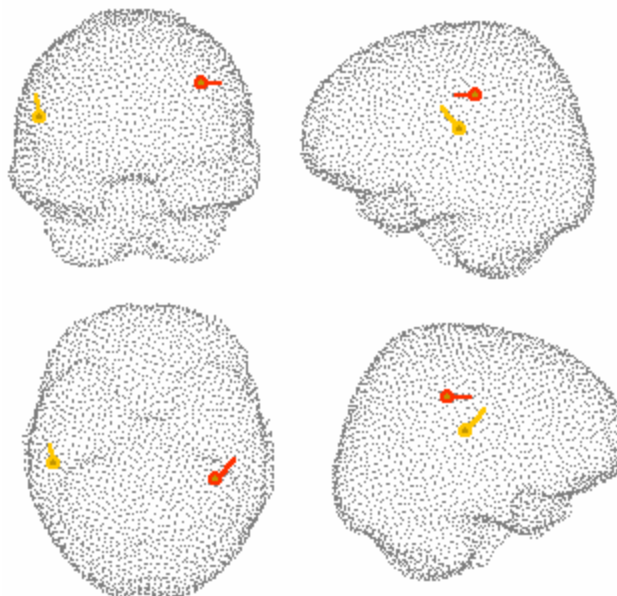
3.2 Example 2

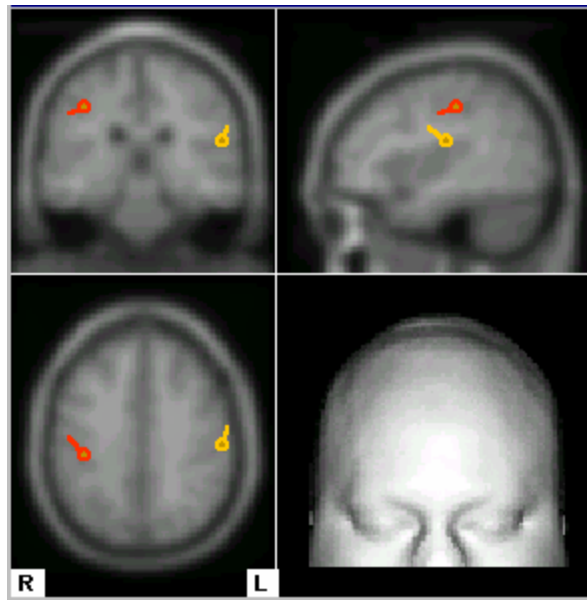
In this example, we will look at the group averaged, auditory evoked responses in a group of adolescent females ($n=5$, ages 14-15). A word list consisting of animate and inanimate objects was presented binaurally. The task was to count the number of words that represented mammals. 64 channels of EEG were recorded. Knowing that there is bilateral temporal lobe processing of auditory stimuli, and that the primary projection areas are relatively focal in comparison to the secondary and tertiary processing areas, we anticipate that a 2 dipole model would be appropriate, and that earlier components (P1 and N1) may have more stable solutions than later components (N2 and P2).

We'll begin with a 2 dipole, Fixed (coh.) model, looking at the interval encompassing the P1 component (28-82ms), using three spherical shells. (Measured electrode position information was not available, so Label Matching was used).

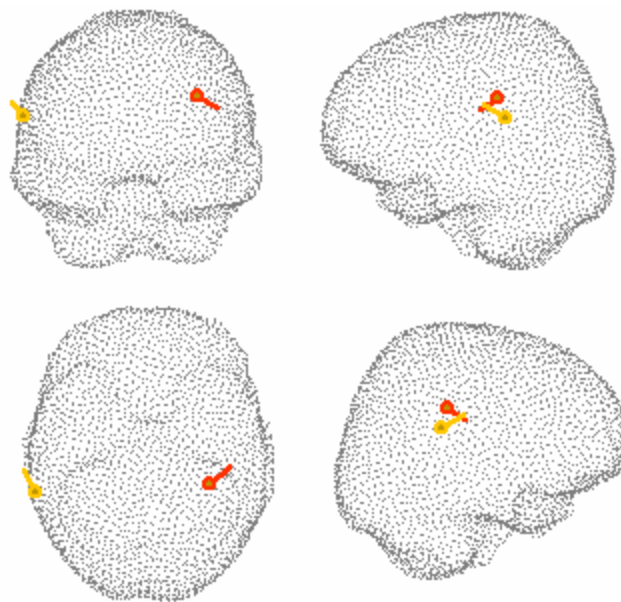


The results show 2 nearly homologous, dipole solutions, which are close to our temporal lobe expectations.

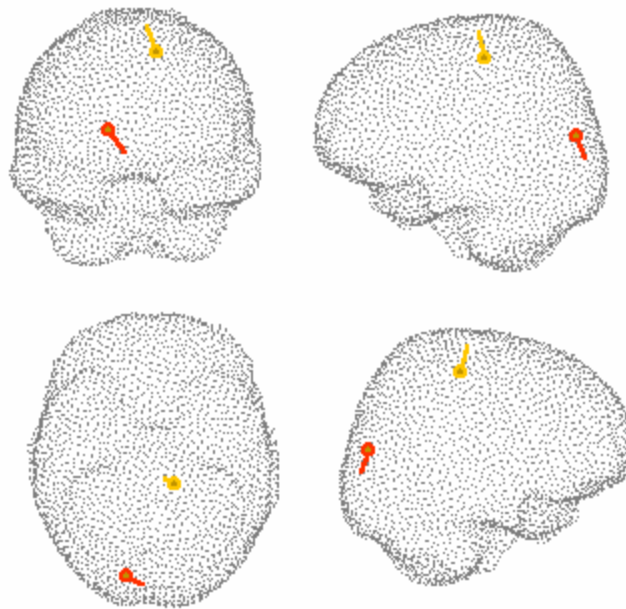
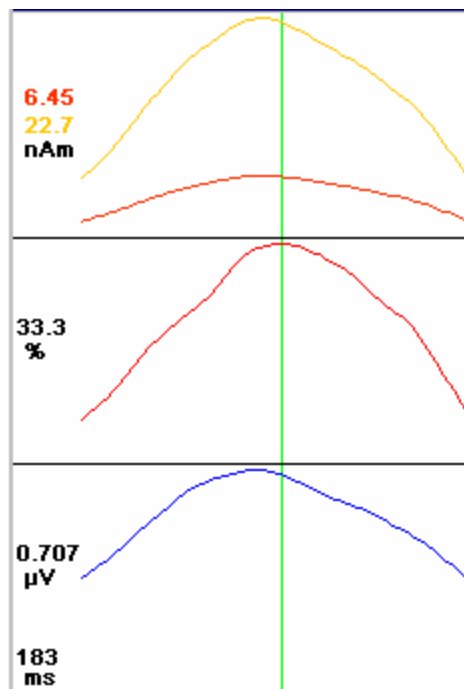




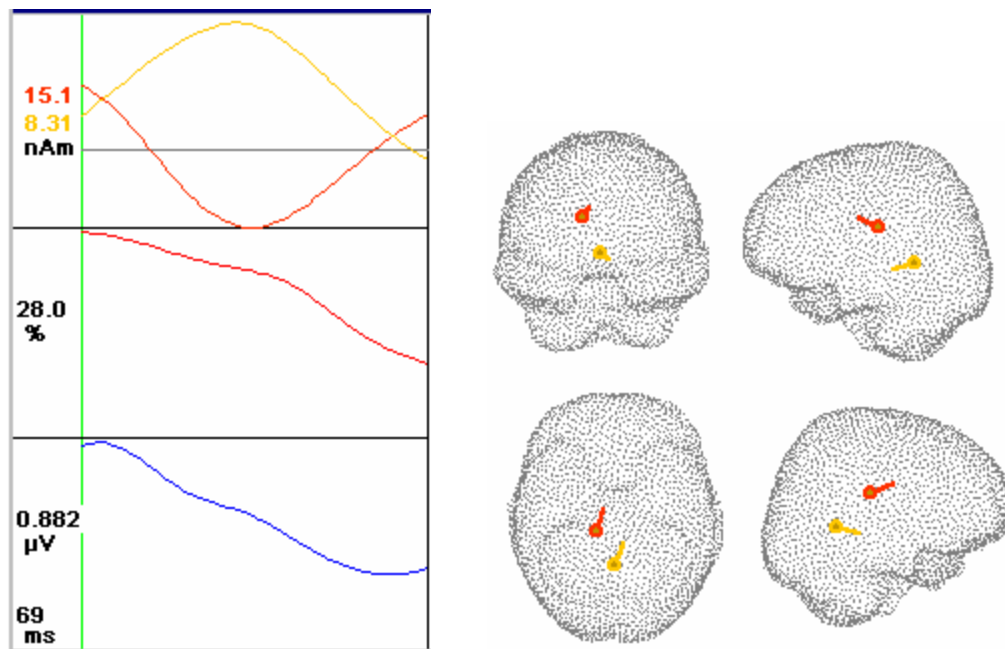
Similarly, the results from the interval containing the N1 component (70-135ms) also indicate 2 nearly homologous sources from the same areas. (The variation from precise expected sources may be due to the lack of measured electrode positions. Source locations should be considered as approximations in these cases).



Looking at the P2 component (135-230ms), however, the solutions become less lateralized. The more prominent one (in yellow) is fairly central, while the weaker dipole shows an unlikely occipitoparietal location. Note also that there is considerable residual deviation, and that the SNR is low. These are not particularly valid looking solutions.



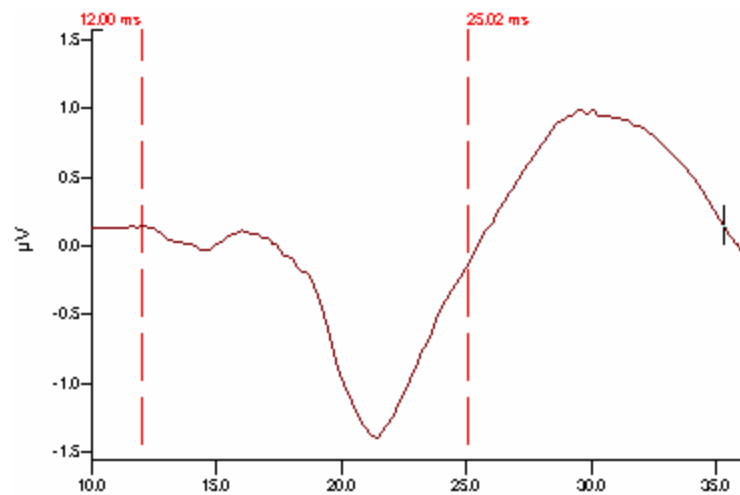
For comparison's sake, we again selected the interval containing the N1 component, and applied the Fixed (MUSIC) model, with 2 dipoles. Very different sources were calculated. Again, the residual deviation is high and the SNR is low, suggesting that these solutions may not be valid.



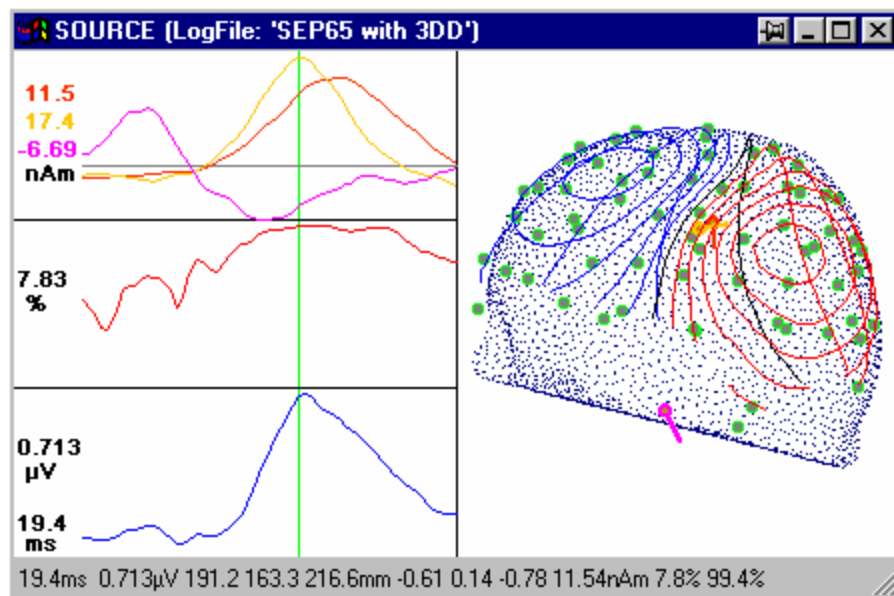
This is in contrast to the results from Example 1 in which the Fixed (MUSIC) solution fit well with the other models, while the Fixed (coh.) model did not. How can this be interpreted? With early somatosensory EP data, for example, one tries to achieve a functional mapping of well localized brain activity. In this case one expects two or perhaps three centers of dipolar activity (depending on the chosen latency range), which can be well represented by two or three fixed (MUSIC) dipole (and not coherent fixed dipoles, because you do not expect coherent activity). AEPs are more difficult to analyze as one may well anticipate simultaneous (coherent), mirrored activity in both hemispheres, which is not quite as well localized as in the SEP case. Later latencies (as with the P2 component above) are almost always more difficult to analyze, since activity has become more diffuse.

3.3 Example 3

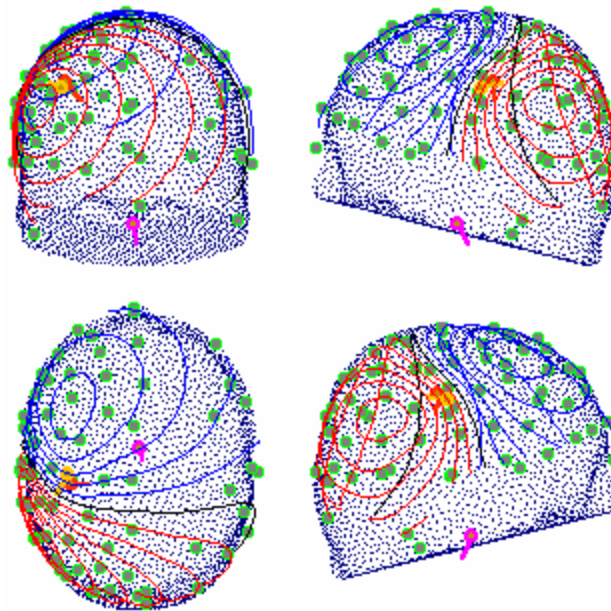
Next, we will look at an SEP recording (right median nerve stimulation). The time interval is 12-25ms, and we used the Fixed (MUSIC) model with three dipoles, and three spherical shells.



The power of the Fixed (MUSIC) source model is demonstrated very nicely. The data exhibit very stable, accurate, and well localized focal sources (a tangential dipole at about 19 ms, a radial dipole at about 21 ms, and the early brainstem activity at about 14 ms).



Below are the same results displayed in four views.



3.4 Example 4

The choice of the volume conductor model you use can affect the source solutions, sometimes dramatically. For the sake of demonstration, we will analyze the same data interval using the four volume conductor models. We will use the *EpiSpike.avg* file, with an interval of 0-50ms, and a Moving dipole model (with a 70% threshold). Selecting the three spherical shell model shows the dipole source localization as displayed below in pink. The red dipoles are using the standard BEM model. Using the BEM model gives results that more closely follow the contour of the temporal lobe.



The solutions with the BEM (pink) and FEM (red) interpolated volume conductor models show results very similar to each other and to the standard BEM model.

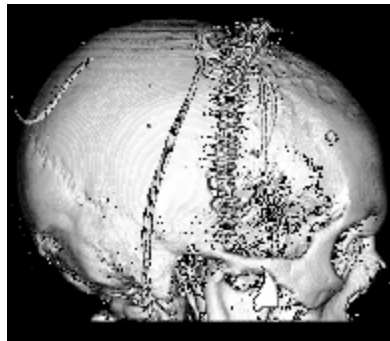
In this example the BEM and FEM models all give comparable solutions, and any of them would be more accurate than the three spherical shells model. In other instances, you may see less subtle differences among the BEM and FEM conductor models, and more consistent results with the three spherical shells model. In general, however, the BEM and FEM models will likely be more accurate than the spherical shells model.



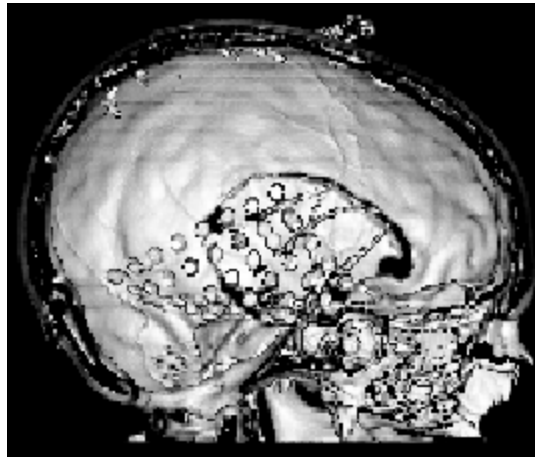
3.5 Example 5

Threshold Segmentation of CT-Image Dataset

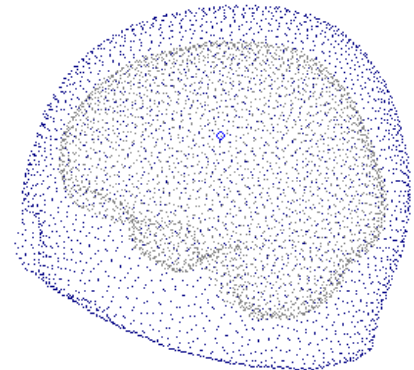
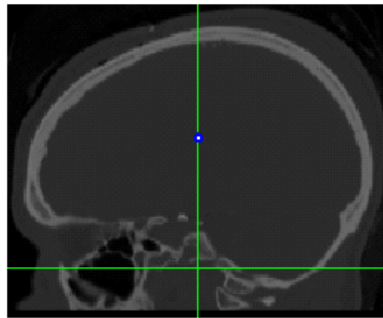
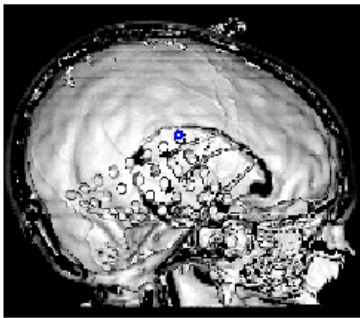
In this example we loaded CT data from a subject with a cortical grid, where we wish to create the actual grid placements. After loading the CT data, rotate the *mouse wheel* (or drag up and down with *right mouse* button pressed) in the SLICE display, and adjust the segmentation threshold from **30** (skin) to about **50** (skull). Change to the **Right View**. There should now be a good view of the skull.



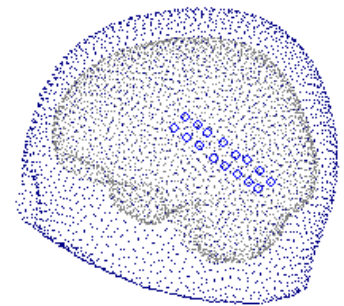
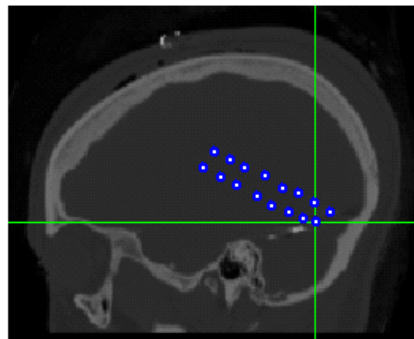
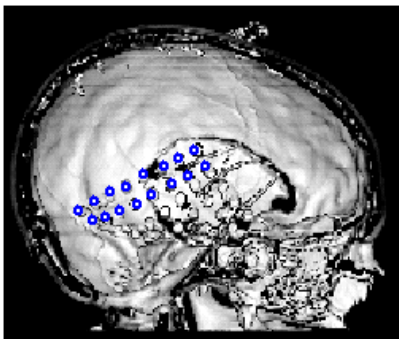
Right click in the display and select **View** → **Cut Right** to see the ECoG grid.



The next step is to determine the depth of the grid electrode positions. To localize the ECoG electrodes, click on an electrode and press **G** (or *right click* and select **Get Position**). This should be done in the same order as the electrodes are labeled in the data file. The position is transferred to the iso-images as well as to the Source display.



Click all of the electrodes in the grid (or as many as desired). Note that there is the option to **Delete Positions** (*right click*, **View** → **Delete Position** or **Delete All Positions**).



The position list can be saved for later use (positions are saved in PAN coordinates; *right click* in the Source display and select **Save Marker Positions As...**). The positions are saved to a .dig file. The .dig file contains the xyz coordinates, as shown, along with the electrode number.


-62.63	16.27	80.52	1
-63.22	6.09	78.06	2
-63.72	-3.08	76.29	3
-64.51	-16.15	72.62	4
-65.13	-24.10	67.97	5
-61.36	-35.33	65.42	6
-51.98	-43.40	61.91	7
-48.15	-51.38	57.86	8
-64.05	19.99	71.94	9
-63.63	8.74	68.73	10
1.58	-4.53	61.69	11
-62.70	-11.20	61.82	12
-64.50	-23.20	58.90	13
-61.68	-31.67	56.78	14
-52.37	-39.89	52.42	15
-43.84	-46.41	52.21	16

The list can be recalled later using **Read Marker Positions**, and the points will be seen in the SOURCE display.

Summary. The above examples demonstrate some of the procedures and interpretational considerations that are used with SOURCE. Depending on the models used, there may be widely varying results. Legitimate applications require careful consideration of the results, validation of findings using different methods, knowledge of the computational differences among the various methods, and a supporting foundation of neuroanatomy and electrophysiology. For more information, see the suggested references.

4 Operating SOURCE

To run the SOURCE program offline, go into EDIT and retrieve an AVG, EEG or CNT file.

You will then notice that the SOURCE icon on the Toolbar will become active . Select one electrode, and enlarge it to midsize or full size (AVG and EEG files). Click the icon and you will see the SOURCE Startup display.



The log file is created when you use SOURCE, and it will contain the electrodes that were used and their 3D positions, the landmark positions that were used, and results from the

analyses you perform in summary form. Subsequent results may be added to the same file. The file can be viewed with a text editor. Use the **Log file** button if you wish to save the analyses you will be performing to a different log file, or type in a different name if you want to create a new log file. A section from a typical log file appears as follows. This is an example of a log file that is produced with moving dipoles, and when confidence ellipsoids (confidence intervals [ci - units: mm and cm³]) are activated (displayed).

```

common BEM scaling factor: 0.989

transform electrodes for BEM model (F2A)

total number of nodes in geometry description: 4656

number of sensors: 1065

maximum distance electrode - projection point: 18.38mm

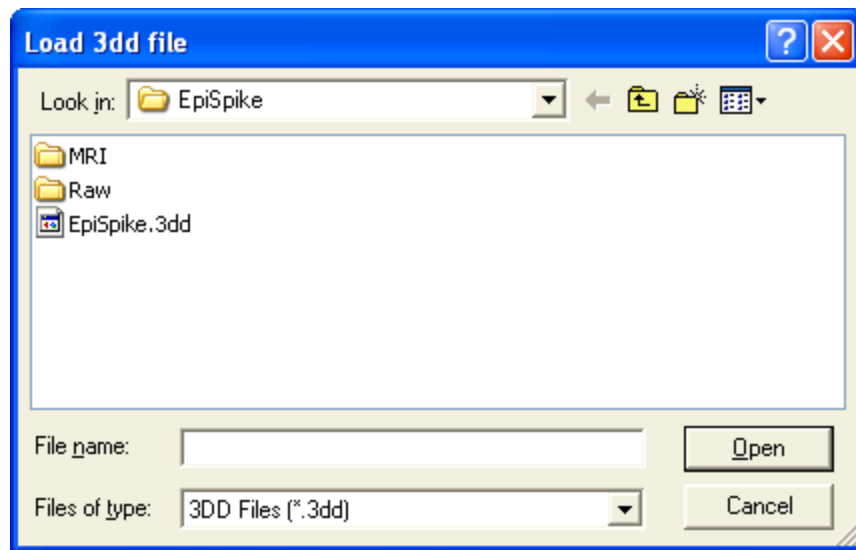
Standardized BEM
moving dipole
-15ms - 55ms best: 20ms 152.9µV
dev var 10.6%, 98.8% [1547ms]
p, n, j: 185.2 -35.5 -81.8, -0.09 -0.96 0.27, 10311nAm, SNR: 10.1, ci: 1.1 4.9 14.1mm, 0.3cm3

latency[ms] MGFP[µV] position[mm] normal strength[nAm] deviation[%] variance[%] SNR confidence axes[mm] volume[cm3]
-15.00 25.36 168.44 -55.13 -90.02 -0.883 -0.090 -0.461 1887 32.1 89.7 1.7 2.8 7.8 64.6 6.0
-10.00 42.16 166.67 -53.83 -100.16 -0.854 -0.005 -0.520 6534 24.9 93.8 2.8 0.7 4.3 25.9 0.4
-5.000 66.71 169.21 -55.47 -110.81 -0.977 -0.144 -0.160 19289 21.3 95.5 4.4 0.3 1.2 23.7 0.0
0.000 92.39 169.33 -55.38 -110.91 -0.981 -0.137 -0.136 22984 18.5 96.6 6.1 0.4 1.7 17.1 0.1
5.000 114.2 168.44 -57.13 -89.71 -0.823 -0.435 0.366 4830 15.2 97.7 7.6 3.0 20.0 27.6 7.0
10.00 131.7 169.99 -42.95 -86.37 -0.399 -0.708 0.582 8853 14.4 97.9 8.7 1.7 10.4 37.1 2.7
15.00 145.1 179.16 -34.83 -83.39 -0.235 -0.857 0.460 10364 12.6 98.4 9.6 1.5 2.1 6.5 0.1
20.00 152.9 185.17 -35.55 -81.85 -0.092 -0.959 0.269 10311 10.8 98.8 10.1 1.1 4.9 14.1 0.3
25.00 153.9 187.67 -36.06 -79.74 0.194 -0.865 0.464 7062 10.9 98.8 10.2 3.5 8.7 23.6 3.0
30.00 146.8 191.05 -41.86 -84.07 0.163 -0.974 0.160 8824 13.4 98.2 9.7 9.6 10.7 15.2 6.5
35.00 130.9 194.73 -47.29 -90.43 0.157 -0.975 0.156 6987 16.1 97.4 8.7 9.8 11.6 21.1 10.0
40.00 107.4 199.90 -52.30 -98.22 0.107 -0.986 0.129 5342 19.0 96.4 7.1 11.1 14.2 27.4 18.1
45.00 79.38 203.30 -57.56 -109.39 0.045 -0.996 0.083 3788 23.6 94.4 5.3 14.9 20.8 33.2 43.1
50.00 52.23 205.74 -81.14 -129.24 0.030 -0.999 -0.030 2331 30.6 90.7 3.5 21.5 29.4 61.5 162.7
55.00 39.50 208.49 -91.37 -136.74 -0.222 -0.687 -0.692 1392 46.2 78.6 2.6 4.9 31.0 40.3 25.7

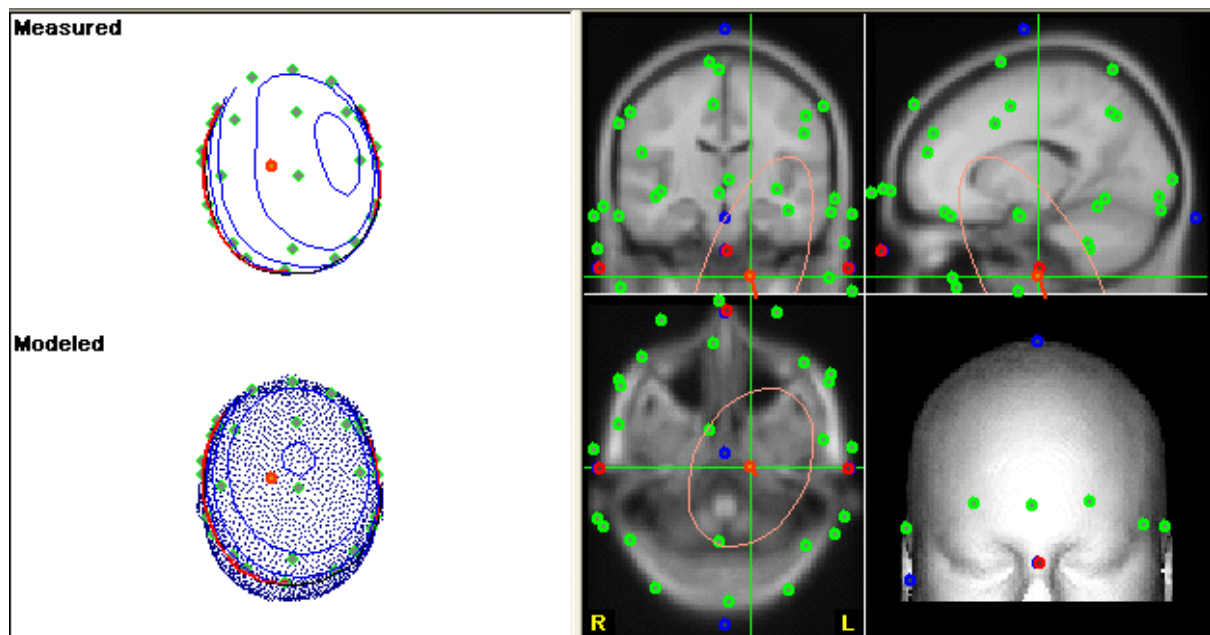
```

The **Match Labels** and **Electrode Positions** fields may or may not be grayed out. If both are grayed out, that means that the program was unable to match any of the labels in your data file (see Appendix A). The **OK** button is also grayed out, leaving you with **Load Positions** and **Cancel** as the only options. Use **Load Positions** to select a 3DD file that matches the data file. If the **Match Labels** field is active, but the **Electrode Positions** field is grayed out, you have the option of using the SOURCE label matching algorithm, or importing your own electrode position data. If you use the **Match Labels** option, SOURCE will attempt to use your existing labels (conventional extended 10-20 system nomenclature; see Appendix A) for placing and fitting your electrodes. If you use conventional labels and do not have their 3D position coordinates, select **Match Labels** and click **OK**.

Whenever possible, you should use the actual measured electrode positions (otherwise you may well introduce unnecessary systematic errors). If you have the actual electrode position information for the data file(s) you will be using, click the **Load Positions** button. (When you close the data file, save the modifications, and the next time you retrieve the same data file the **Electrode Positions** field will be active automatically). You will see the following display. Select the 3DD file (created from 3DSpaceDx) that corresponds to your data file, and then click the **OK** button.



You will then see the SOURCE window appear. The Status bar at the bottom of the SOURCE display will show how many electrodes were matched
 label matching recognized 28 sensors, please select time point (if label matching was used).

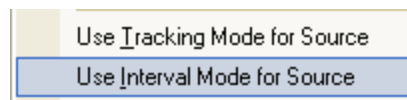


There are two sections to the SOURCE display: the one with Measured/Modeled data, and the one with the MR images. The latter one is referred to as the SLICE display. (Note that you may reposition the vertical bar between the two regions by grabbing and dragging it).

All of the operations may be accessed with the mouse. Many have alternate key board controls (such as, press the *M* key to play a Movie, or the *R* key to perform a Rotation). Keyboard commands are displayed on the right side of the menu lists, as shown in the figure shown.

✓ Contour Lines	C
✓ Electrodes	E
Landmarks	L
Volume Conductor	V
✓ Skin	Alt+S
Skull	Alt+K
Brain	Alt+B
<hr/>	
✓ Conf. Ellipsoids	Alt+C
<hr/>	
✓ Source Waveforms	W
✓ Deviations [%]	Alt+D
✓ MGFP [μ V]	Alt+G
LOG (MGFP)	Alt+O
✓ Min / Max Scaling	Alt+M

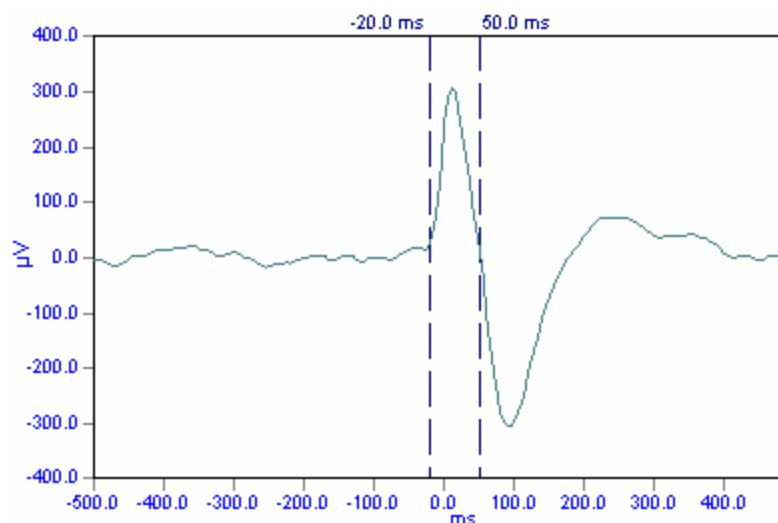
Modes of Operation. SOURCE has two modes of operation - Tracking and Interval. Click the right mouse button in the *data* display (the original waveforms) to see these options.



Use Tracking Mode for Source. When enabled, if you move the mouse within the data display, you will see the corresponding single dipole solution in the SOURCE window. The dipoles are recomputed as the mouse is moved. When Tracking Mode is disabled and Interval Mode is selected, you need to use the left mouse button to drag the cursor to the point of interest in the data file. The corresponding dipole will be displayed in the SOURCE window.

Use Interval Mode for Source. When enabled, you may select the Timerange, or interval for analysis. There are slight differences in how the interval is selected among the types of data files.

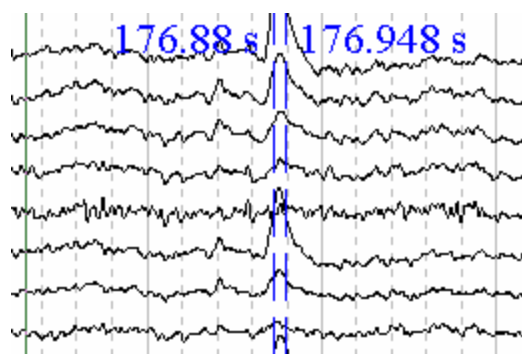
Setting the Interval for AVG or EEG files. With AVG or EEG files, you will see that there are two vertical cursors in the data display window (initially, they may be superimposed). (Note: one of the electrode channels must be enlarged to midsize or full size to see the cursors). Use the left mouse to grab and drag them. If both cursors move together, one will be "dropped" when you reverse direction.




The cursor positions may be controlled by the mouse or by the arrow keys on the keyboard. The arrow keys by themselves move the left cursor. Using the *Shift* + *arrow* keys moves the right cursor. The *Ctrl* + *arrow* keys will move both cursors together, keeping the same interval between them.

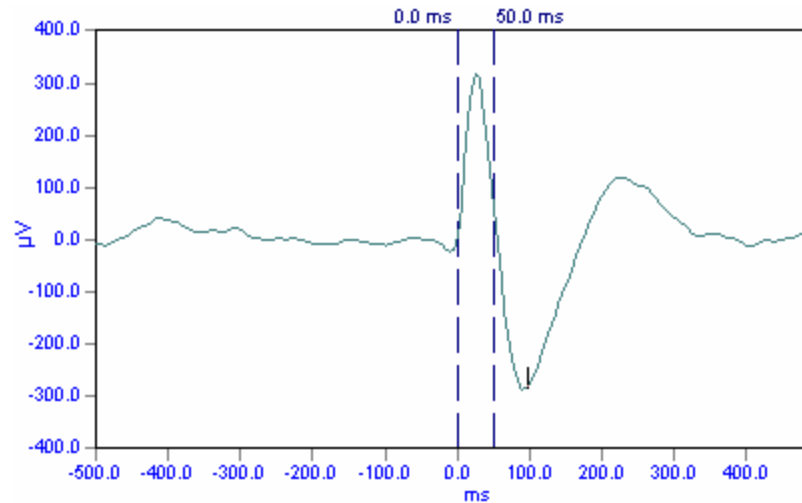
When you have retrieved an EEG file, and you wish to move to a different sweep, just close the full-sized channel display and the arrow keys will have their normal functions returned.

Setting the Interval for CNT files. To select the interval for analysis with CNT files, click the right mouse inside the data display window and enable the **Use Interval Mode for Source** option. You will see two colored, dashed vertical lines (they may initially be superimposed) in the Single Window display, with the latency (seconds into the file) showing. Grab and drag these to the desired interval. The analyses will then be computed using the interval.



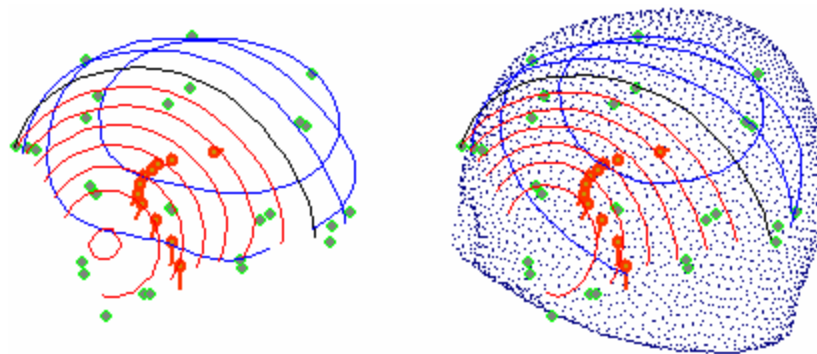
Note: You may change the color of the cursor by selecting Options, Single Windows Settings. The Cursor option may be used to select the color.

For example, retrieve the *EpiSpike.avg* file that was installed into the ...\\Scan Data\\Demo Files\\EEGSpikes folder. Make one of the channels full size (such as F7), and click the SOURCE icon . From the SOURCE Startup screen, load the *EpiSpike.3dd* electrode position file. Enable the **Use Interval Mode for Source** option, if needed. Position the cursors to define the approximate 0-50ms interval (F7 channel shown).

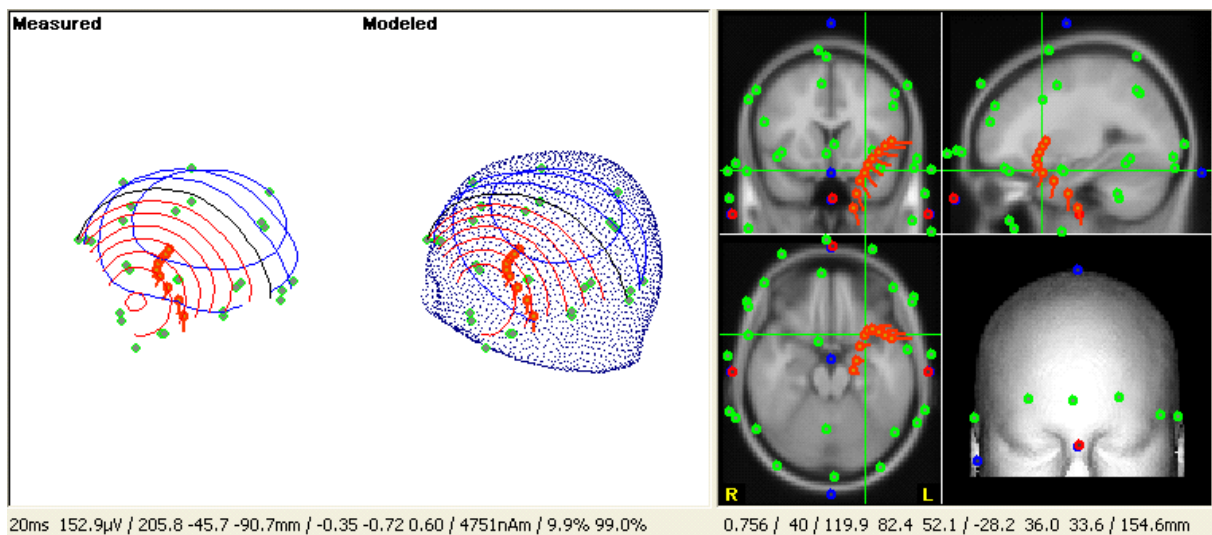


By default, the results for the Moving Dipole solution are displayed in the SOURCE screen. To change the size of the images in the SOURCE display, simply rotate the mouse wheel or hold down the right mouse button while moving the cursor.

The results are also displayed on a generic MRI head (shown below). You may change the levels of the slices in any of the perspectives by clicking the left mouse button to the desired point in one of the cross-section displays, or, you may grab and drag the "cross-hair" to a desired location. Moving the crosshair in one display will shift the level of the slice in the other two cross-section displays.



SOURCE Status Bar. On the Status bar at the bottom of the SOURCE display, you will see a series of numbers.



The first set of values is associated with the SOURCE display.

The first number is the time point in the interval that has the least value in the Deviations function (the "best fit" latency). After an analysis has been run, the program will return to this point automatically.

The second number is the Mean Global Field Power (MGFP) value, taken from the same time point in the interval (a measure of signal strength).

The next three numbers are the fitted dipole coordinates (in mm).

The next three numbers are the dipole orientation values (unit vector).

The ninth number is the dipole strength (in nAm) at the indicated time point in the interval.

The tenth number is the fit quality in % residual standard deviation. Square that number $[(9.9/100)^2 = \text{approx. } 1\%]$ and subtract it from 100% to get the % explained variance.

The final number is the % explained variance.

The second set of values is associated with the SLICE display.

0.756 / 40 / 119.9 82.4 52.1 / -28.2 36.0 33.6 / 154.6mm

The first number is the Scaling factor, or the number of screen pixels per mm. This can be changed by resizing the whole window.

The second number is the threshold value for surface rendering in rendering mode. This can be changed by rotating the *mouse wheel*, or by holding down the *right mouse* button while moving the cursor. If you are in **Maximum IP** mode, this number is the grayscale value (also may be changed by rotating the *mouse wheel*, or by holding down the *right mouse* button while moving the cursor). Both of these numbers may be set from the Image Parameters screen (*right click* in the SLICE region of the window and select **Data Parameters**).

Threshold / Grayscale		
Threshold:	<input type="text" value="40"/>	Grayvalues: Lower <input type="text" value="0"/> Upper <input type="text" value="255"/>

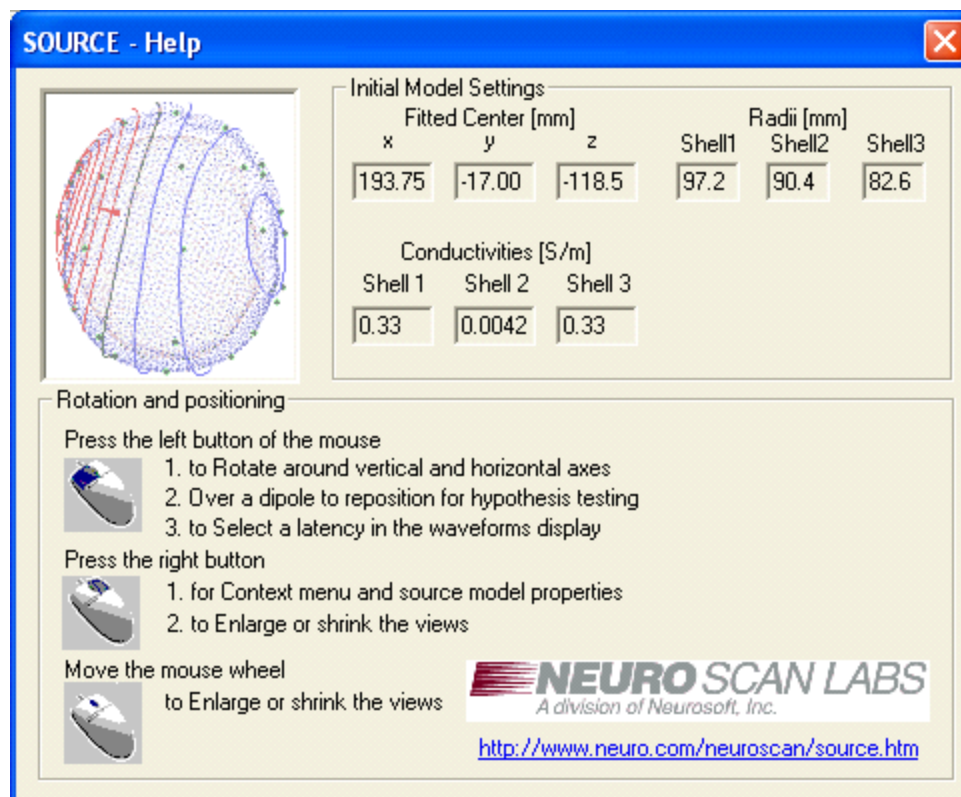
The next three numbers are the x- y- z- coordinates in the image coordinate system (mm). X: right -> left, y: front -> back, z: bottom -> top. The origin is in the lower right frontal corner.

The next three numbers are the x- y- z- coordinates in the PAN coordinate system (mm), if all anatomical landmarks are set.

The last number is the distance from the reference point to the actual cursor position (mm). The Reference point can be set by pressing *R*, or by *right clicking* in the SLICE region, and selecting **Set Reference**. This is discussed more fully in the Set Reference / Show Reference section below.

4.1 SOURCE Help screen

Click the *right mouse* button inside the SOURCE display, and click **Help** from the list of options. You will see the following screen.



The upper part of the display shows the XYZ coordinates for the Fitted Center (in mm's), the Radii (in mm's) for the three concentric shells, and the Conductivities for the three concentric shells. The outermost shell (the skin) is fitted to all used electrodes, and the inner shells are at 93% (outer skull compartment) and 85% (inner skull, or brain compartment) of the outermost radius. These values, as well as the Conductivities, can

be overwritten manually (described below). The coordinate system for the Fitted Center is the same system used with the electrode position coordinates.

The lower part of the display describes the function of the mouse buttons and the mouse wheel. Uses of the mouse buttons and wheel will be discussed more below.

4.2 SLICE Help screen

A different Help screen will be shown if you select **Help** from the SLICE display (using the *right mouse* options from that part of the display).

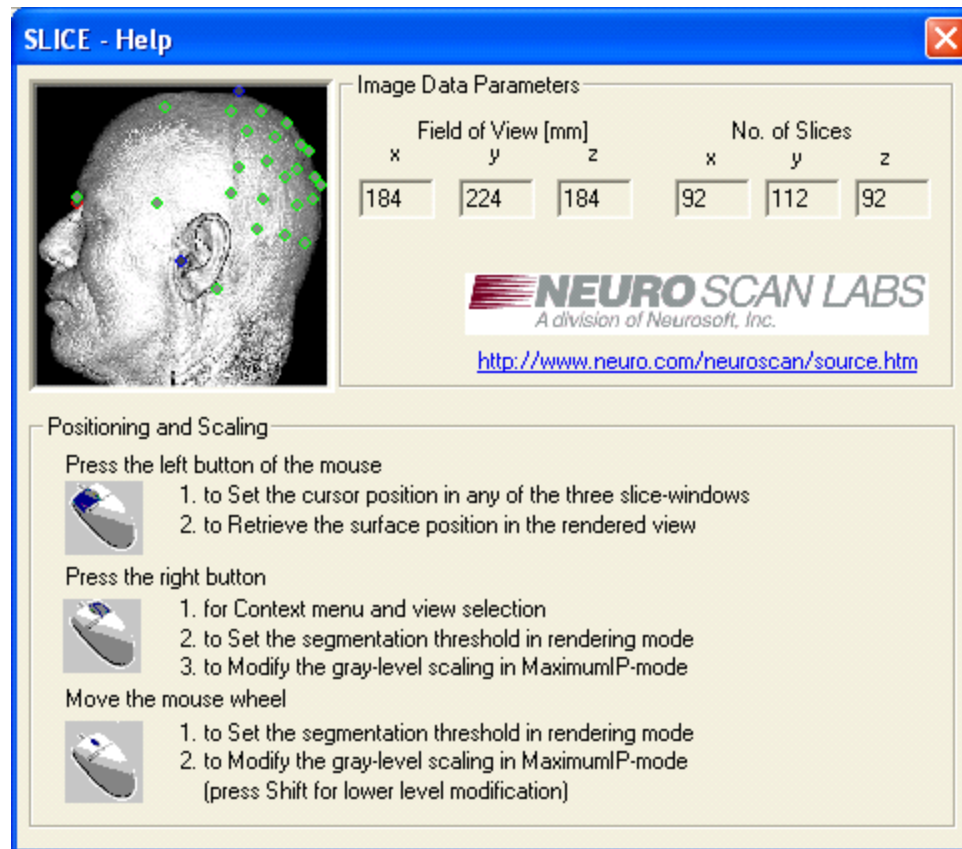


Image Data Parameters. This group of fields displays the maximum value for the Field of View [mm] for the three axes, and it displays the number of slices along each axis.

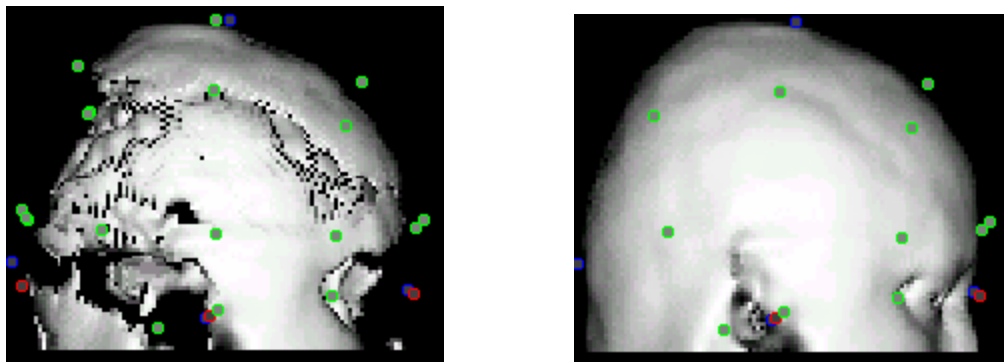
Positioning and Scaling. The information summarizes the functions of the left and right mouse buttons, and the mouse wheel.

Left mouse button. The left mouse is used primarily to position the crosshairs in any of the three slice windows. Click it in the rendered view (the lower right image) to set the crosshair on a desired point on the surface.

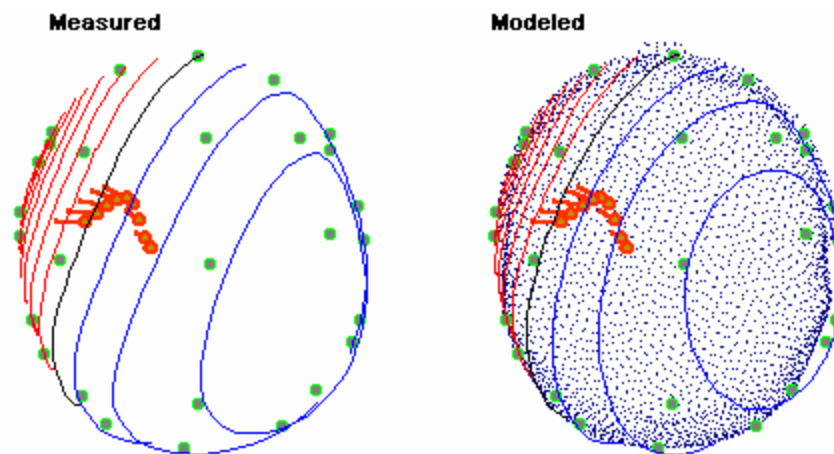
Right mouse button. The right mouse button is used to display the Option menu for the SLICE window (described in more detail below). It can also be used in place of the mouse wheel. For example, click and hold the right button down in the SLICE

rendered view, and then move the mouse to adjust the segmentation threshold (see the next figure). In Maximum IP mode, the same operation will modify the graylevel scaling. You can change the start value by holding the Shift key down while dragging the cursor with the right mouse button (see the second set of numbers on the SLICE part of the Status Bar). In the SOURCE part of the display (the Measured and Modeled data display), you can zoom in and out by dragging (vertically) the cursor with the right mouse button.

Mouse wheel. Rotate the mouse wheel to vary the segmentation threshold in the rendered image. The default settings are correct for the generic head shape; however, if you import your own MRI data, you may find that you need to adjust the segmentation threshold. The figures below show an example (left) where the threshold was set too high, and the skin surface has been eroded away. The example on the right shows the same data with the correct threshold. If the threshold is set too low, the surface electrodes will disappear.



The wheel is also used to vary the graylevel scaling in *Maximum IP* mode. To do this, click the *Maximum IP* option from the right mouse accessed Option list. Then rotate the wheel by itself to vary the intensity of the white end of the gray scale. Hold the Shift key down and rotate the wheel to vary the black end of the gray scale. Click the *Reset Grayscale* option to return to the default levels. In the SOURCE part of the display (the Measured and Modeled data display), you can zoom in and out by rotating the wheel.



Looking again at the SOURCE display, it is possible to change the perspective of the image

in several ways (described below). The SLICE display above was from the right side. The contour display to the right is a top view. In this example, a Moving Dipole model was used, and you can see the dipole source solutions as they vary as a function of time. The display on the left shows the *Measured* data contour (equipotential) lines, electrodes, and the dipole locations. The image on the right displays the *Modeled* potential contour lines, electrodes, and dipole location. In this figure, the skin point cloud is displayed - you can also show the skull and/or brain point clouds, and other information, as described below.

4.3 The Option Menu for Source

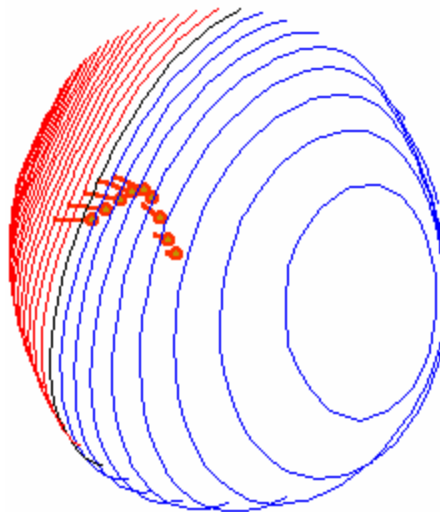
The Option Menu for Source. All of the display and analysis options may be selected from the context menu, seen by clicking the *right mouse* button within the SOURCE display.

Display	►
View	►
Movie	M
Save Movie As...	Ctrl+O
Rotation (360 deg.)	R
Save Rotation As...	Ctrl+T
Copy To Clipboard	Ctrl+C
Save As (*.bmp, *.emf)...	Ctrl+A
Print...	Ctrl+P
Colors...	Ctrl+L
PAN Coordinates	Alt+P
Save Marker Positions As...	Ctrl+V
Read Marker Positions...	Ctrl+E
Use Markers As Seedpoints	Ctrl+U
Help...	F1
Source Parameters...	P

Display options. The first twelve options let you select what information is to be displayed. You may select any, all, or none of the options (selecting none of them displays the dipole solution only).

✓ Contour Lines	C
✓ Electrodes	E
Landmarks	L
Volume Conductor	V
✓ Skin	Alt+S
Skull	Alt+K
Brain	Alt+B
Conf. Ellipsoids	Alt+C
✓ Source Waveforms	W
✓ Deviations [%]	Alt+D
✓ MGFP [μ V]	Alt+G
LOG (MGFP)	Alt+O
✓ Min / Max Scaling	Alt+M

Contour Lines. The Contour lines are equipotential lines, where the blue lines are negative voltages and the red lines are positive voltages. The black line is the zero potential line.

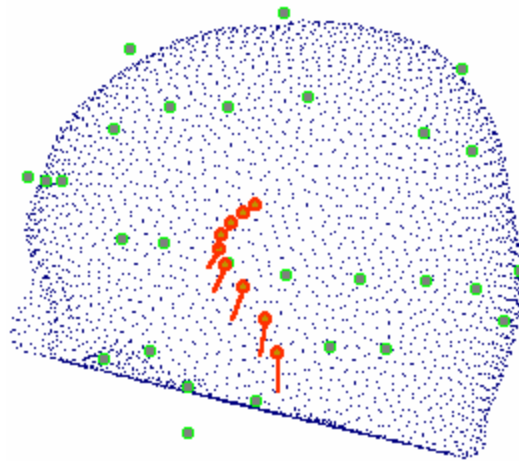


The Contour Interval can be varied by clicking the *right mouse* button, then selecting **Source Parameters**, then changing the interval using the up and down arrows in the

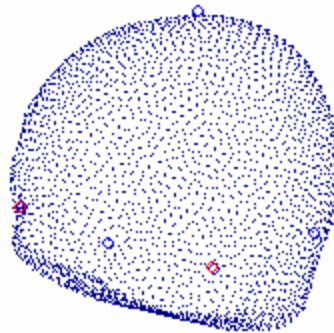
Contour Increment field contour increment [μ V]. Click **Apply** to see the new contours (you do not have to close the Parameters window). An easier way is to use the up and down arrows on the keyboard to change the contour interval.

Electrodes. Enabling this option will display the positions of the electrodes (green dots).

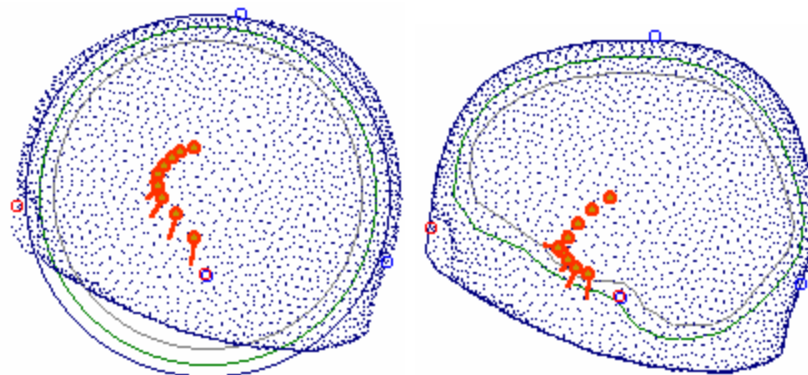
In the picture below, the Skin was enabled also to provide a source of reference.



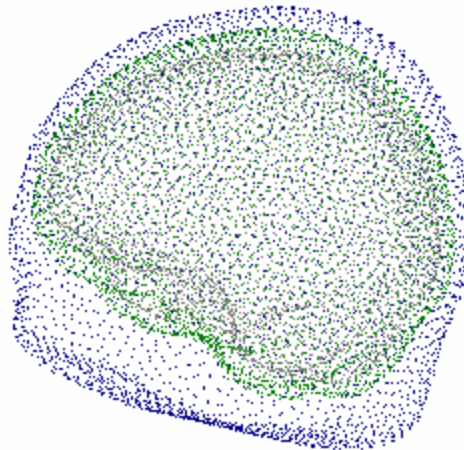
Landmarks. Enabling this option will display the Functional (red) and Anatomical (blue) landmarks. The figure to the right shows the left and right preauricular points and the nasion (red/blue circles), and the vertex and inion anatomical landmarks (blue circles).



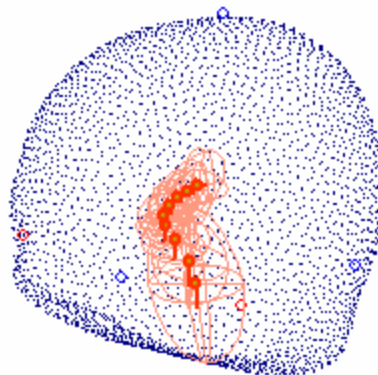
Volume Conductor. Enabling this option will display the three concentric spheres or the BEM or FEM models used in the dipole models.



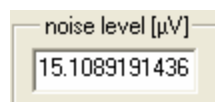
Skin, Skull, and Brain. These toggle on and off the display of the generic Skin, Skull and Brain point clouds.



Conf. Ellipsoids. This toggle is used to display the confidence interval ellipsoids for each dipole solution that is displayed. The "tighter" the confidence interval (i.e., the smaller the ellipsoid), the more certain the location of the dipole. The size of the ellipsoid (the lengths of the axes) is inversely proportional to the SNR, and directly proportional to the estimated noise level. The confidence volume, therefore, is proportional to the third power of the noise.



The estimated noise level is computed automatically (the average of the prestimulus interval MGFP values), and is displayed in the SOURCE Parameters screen, described below.

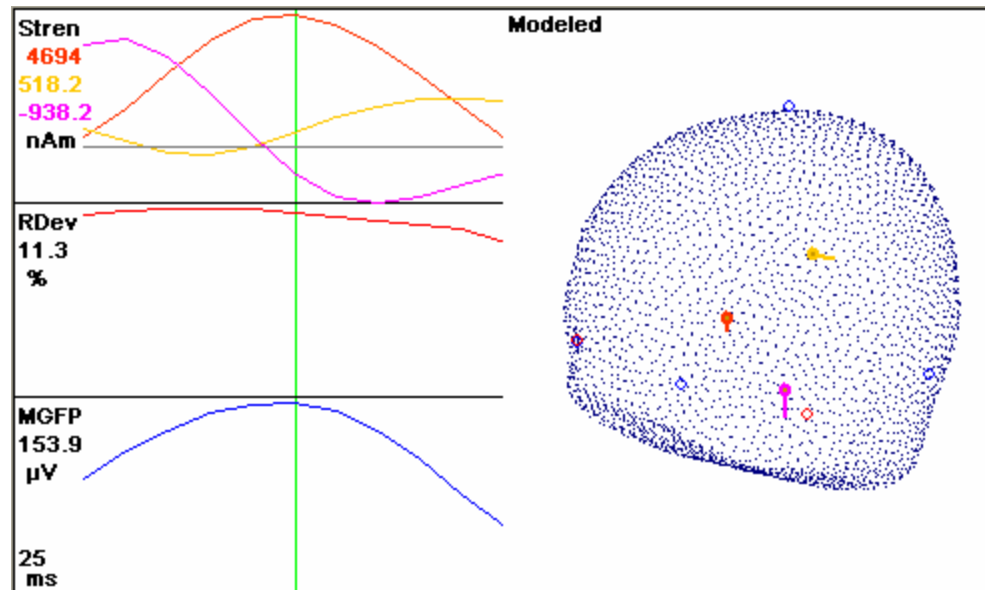


The estimated noise level is assumed to be constant across the time range (stationary). You can use the estimated noise value, or other noise estimate, if desired. If you enter a peak value of noise, then the ellipsoid size is also the peak size.

The confidence ellipsoids give meaningful results only when the correct volume conductor and correct source model are chosen. On the other hand, they can help to determine what the best source model is, since superfluous sources exhibit large confidence volumes (if one dipole is able to explain the data, then a second one, of

smaller strength, can be located anywhere without improving the fit result). The ellipsoids also help determine how meaningful multiple dipoles can be.

Source Waveforms. The Source Waveforms window displays the dipole strength (**Stren**) results for the selected time range. Enable this option to see the waveform displays of the Deviations (**RDev**) and Mean Global Field Power (**MGFP**). Note that these options become active when you enable the **Source Waveforms** option, and you may select either or both of them. The Source Waveforms are the ones in the top region left side of the following figure.



In this example, three dipoles were computed, and the **Min / Max Scaling** was disabled (so all three source waveforms will be superimposed).

Deviations [%]. The Deviations (D, or standard deviation) is a measure for the fit quality (how well the source model explains the measured data). It is the middle region on the left in the figure above (RDev). (Notice that the Y-axis is inverted; that is, the numbers get smaller as you go higher on the graph).

D is the root mean square of the difference between measured (R_i) and calculated signals (F_i):

$$D = \sqrt{1/n * \sum ((R_i - F_i) * (R_i - F_i)) / MGFP}$$

$$= \sqrt{\sum ((R_i - F_i) * (R_i - F_i)) / \sum (R_i * R_i)}$$

normalized for the measured field (MGFP), which corresponds better to the Signal-to-Noise ratio (SNR) than variances.

The residual (or "rest") variance V is simply the square of the standard deviation:

$$V = D * D = \sum ((R_i - F_i) * (R_i - F_i)) / \sum (R_i * R_i)$$

The explained variance is 1 minus the residual variance: $EV = 1 - V$.

MGFP [μV]. MGFP (mean global field power) is a commonly used measure to enable a

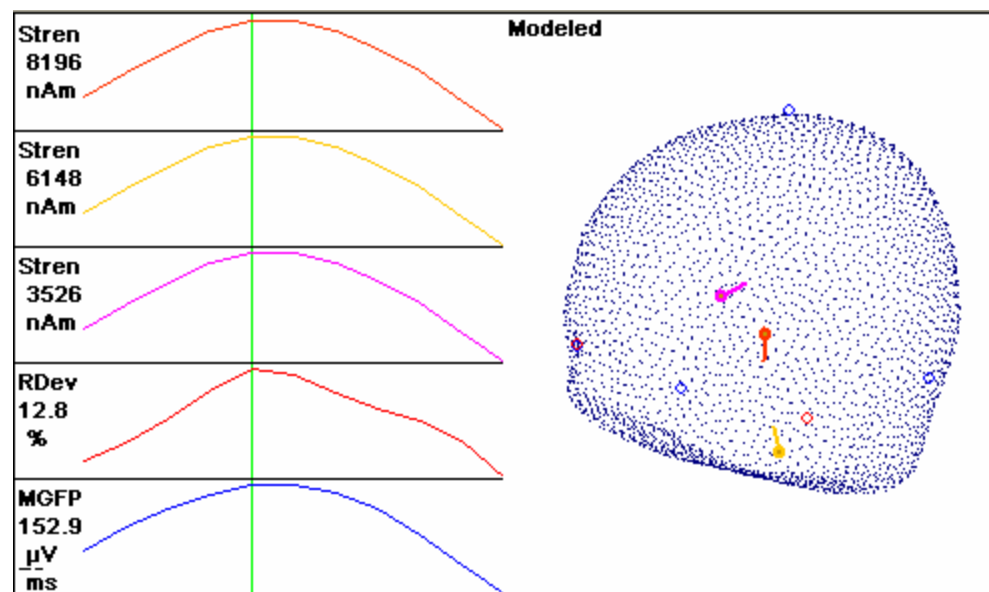
quick overview of the measured EEG time courses, since it collapses the information of all electrodes into a single trace. It is displayed in the lower region on the left in the figure above. As the name suggests, the MGFP is an average of the (common average re-referenced) data. The MGFP is an averaged measure for the signal strength (and thus the Signal to Noise Ratio, or SNR). One can easily distinguish latency ranges with meaningful signal from noise or background activity periods. Estimating the SNR from the MGFP together with the Deviations percentage can tell you if the chosen source model is at least able to explain the signal part of your data.

The MGFP is computed as follows. Let S_i be the measured data ($i = 1 \dots n$ {n electrodes}, for a given timepoint). The common average C is: $C = 1 / n * \text{Sum} (S_i)$, the rereferenced measured data $R_i = S_i - C$. $\text{MGFP} = \text{Sqrt} [1 / n * \text{Sum} (R_i * R_i)]$.

LOG (MGFP). Toggle this on to display the log of the MGFP values.

Min / Max Scaling. Min / Max Scaling (*Alt+M*) allows you to switch between autoscaled Minimum - Maximum scales for all traces and a common scale for all dipole loadings (strengths), and 0 - Maximum scaling for the other traces (Deviations and MGFP).

In the example below, **3 Fixed (coh.)** dipoles were calculated, and **Min / Max Scaling** was enabled. The strengths of the 3 dipoles are displayed separately (and are color coded with the dipoles in the *fitted* display). Grab the vertical green cursor with the left mouse button to drag it to any desired location (note that the SOURCE display will show the results for the corresponding time point). You may also use the left and right arrows from the keyboard to move the cursor. If you disable Min / Max Scaling, the Source waveforms will be superimposed with a common scaling.



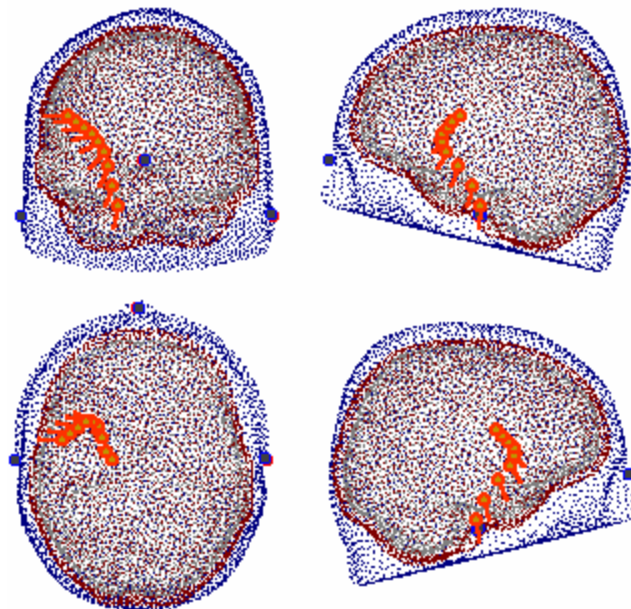
Interpreting the functions. The Source Waveforms, Deviations, and MGFP functions are useful in helping you determine if the dipole solution is a valid one. Loosely stated, the Source Waveforms show the strength and time course of the dipole(s). The Deviations function displays the residual standard deviation. MGFP is a composite measure that indicates the strength of the signal against the noise background. For a

valid dipole, you would expect to see, during the approximate same time course, a strong dipole (peak in the Source Waveforms), low residual or unexplained standard deviation (displayed as a peak in the Deviations function), and a good signal to noise ratio (peak in the MGFP function). In other words, you would expect to see approximately concurrent peaks among the three measures. There are no hard and fast rules as to how strong the dipole must be, how low the residual standard deviation must be (less than 10% is good), or how high the SNR (from MGFP) must be. This becomes a subjective determination, influenced also by the physical location of the dipole solution(s), and by your *a priori* expectations. Obviously, a source located outside the head is not a valid solution. Similarly, an occipital lobe solution for an early SEP component is not valid. Solutions based on Label Matching and the generic MR head shape will not be as precise as those with measured electrode positions and the subject's own MR images.

View options. The viewing perspective may be changed either by selecting a viewing angle from the context menu, or by grabbing and moving the display with the mouse.

Front View	Alt+F
Left View	Alt+L
Right View	Alt+R
Top View	Alt+T
Back View	Alt+V
Four Views	Alt+4
✓ Front <-> Back	F
✓ Tilt View	T

Fixed view positions. From the context menu, you may select to display Front, Left, Right, Top or Back views. Or, you may "grab" the display using the left mouse button, and spin/rotate it to any desired perspective. There is also the option to display Four Views, as shown to the right.



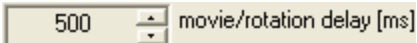
Front <-> Back. The Front <-> Back option reverses front and back for whatever perspective is displayed.

Tilt View. The Tilt View option tilts the display upward by about 20 degrees.

Movie/Rotation options. Next on the *right mouse* option list are the Movie and Rotation options.

Movie	M
Save Movie As...	Ctrl+O
Rotation (360 deg.)	R
Save Rotation As...	Ctrl+T

Movie. Dipole source solutions are calculated for each data point in the defined interval. When you select the Movie option, the dipoles will be displayed at each point through the interval (or press the *M* key). This will let you see the movement of the dipole and/or the changes in the contour lines, depending on which dipole model you have selected. The rate at which the Movie is played is controlled by

the  field on the Source Parameters display. If you want to control the movements manually, select the Source Waveforms option below. A green vertical cursor will appear in the waveform display. Grab this with the left mouse button and move it manually through the interval to see the dipole movement at a desired speed, or use the keyboard arrows to step through the interval. After a movie, the time cursor returns to the best fit latency. Movies may be saved using the **Save Movie As** option described below.

Save Movie As. This option allows you to save the Movie (described above) as an AVI file. Clicking it displays the standard Save As utility. Note: the movies are sequences of individual screen shots, and the movie files can get *very large*.

Rotation (360 deg.). The Rotation option will rotate the display one time through 360 degrees (or press the *R* key). The rate of the rotation is controlled by the

 field in the Source Parameters display. The rotation movie may be saved using the **Save Rotation As** option described below.

Save Rotation As. This option allows you to save the Rotation (described above) as an AVI file. Clicking it displays the standard Save As utility. Note: the rotation movies are sequences of individual screen shots, and the movie files can get *very large*.

Miscellaneous options. The following right mouse options pertain to copying the display with the focus to the Windows[®] clipboard, saving graphic screens, and printing.

Copy To Clipboard	Ctrl+C
Save As (*.bmp, *.emf)...	Ctrl+A
Print...	Ctrl+P
Colors...	Ctrl+L

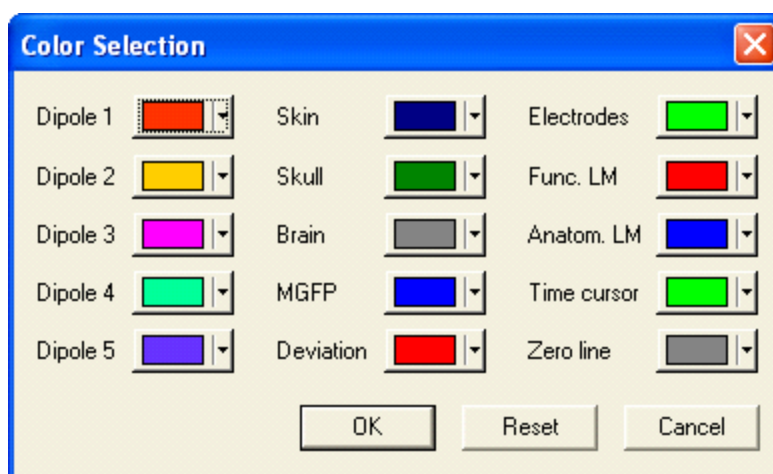
Copy to Clipboard. Selecting this option will copy the highlighted display to the

Windows[®] clipboard (where it may be pasted in other Windows applications, such as Paint).

Save As (*.bmp, *.emf). Selecting this option opens a standard Save As utility, in which you may save the contents of the highlighted display as a .bmp or .emf file.

Print. The Print option displays the standard printing screen in Windows[®]. The contents of the SOURCE display will be printed.

Colors. The Colors option lets you select colors for the dipoles and the other display components as indicated. Select colors as desired. The **Reset** button will return all colors to the default selections.



PAN Coordinates. The PAN Coordinates toggle PAN Coordinates Alt+P (Preauricular points / Nasion) allows you to switch between the PAN system (assuming that at least the left and right preauricular points and nasion have been recorded), and the original coordinate system (the electrodes and the landmarks). In the PAN system, the x-axis goes from the left to the right preauricular point. The y-axis goes from the inion to the nasion, and is perpendicular to the x-axis (pointing to the front of the head, and intersecting PAL-PAR at the halfway point). The z-axis points upwards and is perpendicular to the x- and y-axes. (Enable the option and see the changes in the dipole position and orientation in the status bar at the bottom of the SOURCE display).

Save/Read Marker Positions, Use Marker Positions As Seedpoints. Marker positions are obtained using the **Get Positions** option from the SLICE context menu. When at least one position has been obtained, the Save Marker Positions As option becomes active. Clicking it allows you to save the positions to an ASCII file, with a .dig extension. The files contains the X, Y, Z coordinates for the positions you select.

Save Marker Positions As...	Ctrl+V
Read Marker Positions...	Ctrl+E
Use Markers As Seedpoints	Ctrl+U

The Read Marker Positions option is used to retrieve the marker file. If you then select the Use Markers As Seedpoints option, the point(s) is then used as the starting point for the simplex algorithm optimizer, and the results are then displayed. In practice, it follows that the number of points should be equal to (or less than) the number of dipoles selected for the dipole source model. (For example, if you are solving for two rotating dipoles, you should select two seedpoints for the optimizer starting points).

46.50	-40.15	17.35	1
46.50	-14.22	9.50	2

Help. Clicking the Help option displays the Help screen (described above).

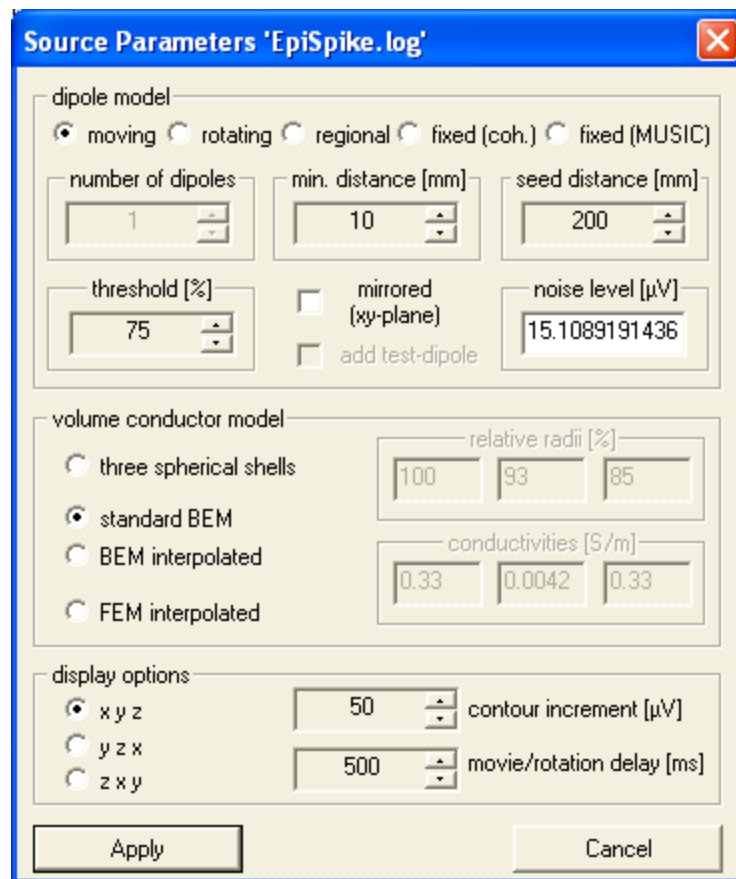
4.3.1 Source Parameters

The Source Parameters

Source Parameters...	P
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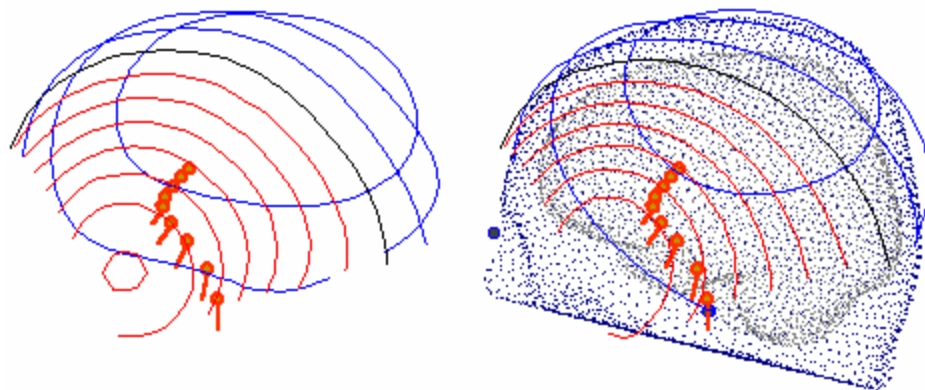
 display lets you select the dipole model that you wish to use, as well as other parameters.

Dipole Models. The dipole model section shows the source models that may be selected. You have the option of selecting a single time point or a latency range for analyses. If you select a single time point, all of the models will produce the same results. If you select a latency range (by positioning the vertical cursors in the data display window), then the models will show differences.



Note: You may select or vary any of the options in the Source Parameters display, and see the effects by clicking Apply, without closing the Source Parameters window. The Options menu (right mouse button) will remain accessible while the Source Parameters display is seen.

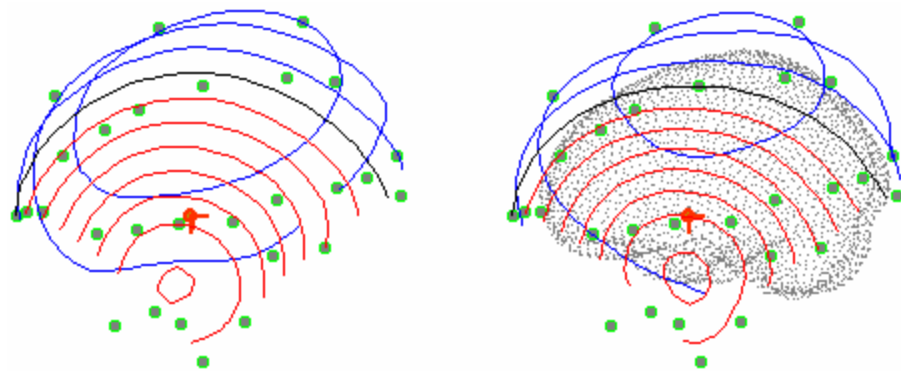
Moving. Moving dipoles may be displayed as a trace, as seen below, or as a Movie (as described above).



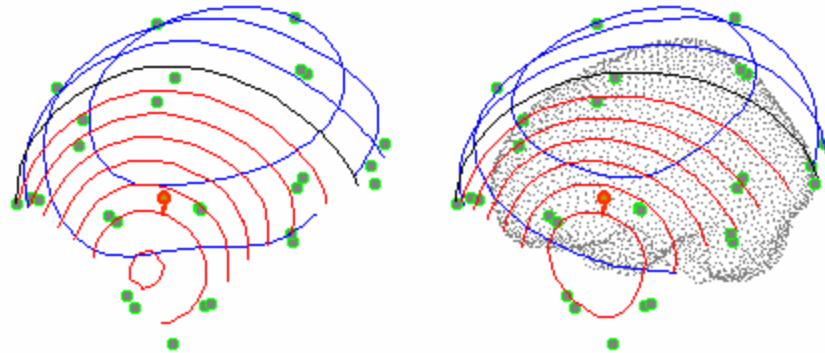
The dipole positions (the nonlinear parameters), orientations and strengths (the linear parameters) for every time point are calculated independently.

Rotating. For a rotating dipole, a common position for all time points is fitted, and the orientation and strength for every time point are calculated, so a rotating orientation may result. The results below are for the same file during the same latency range. If played as a Movie, the orientation would appear to rotate over time.

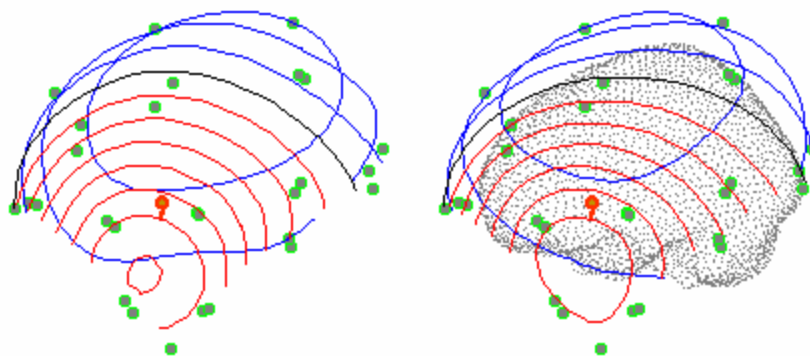
Regional. A Regional dipole is a rotating dipole with an additional postprocessing step. A Singular Value Decomposition (SVD) is applied to each rotating dipole in order to determine its preferred orientation and the two other orthogonal components. Thus, three fixed orthogonal components are obtained per rotating dipole, and their strengths are computed as a function of time (in the waveforms display). (The Regional option was included to provide comparability to BESA results).



Fixed (coh.). For fixed (coherent) dipole, a common position and orientation for all time points is fitted, and the dipole strengths for every time point are calculated. If more than one dipole is fitted, they will all have coherent loadings (same temporal behavior).



Fixed (MUSIC). For fixed (MUSIC) dipoles, the dipoles are fitted recursively using the MUSIC metric, thus coherent sources cannot be separated. The results in this example are virtually identical to the Fixed (coh) model.



Number of Dipoles. The number of fitted dipoles can be adjusted (for moving dipoles without mirror constraint, only one dipole is possible).

Min distance [mm]. For more than one dipole, a minimum distance between the dipole positions can be chosen to avoid strong opposing (canceling) source configurations.

Seed distance [mm]. The seed distance is the maximum distance from the start point (seed) of the dipole fit. The default distance is large - 200 mms - to include the entire head.

Threshold. The Threshold field is active with Moving dipoles only. This parameter may be used to suppress bad fit results (e.g., at latencies with low SNRs). If you select a large time range, and set the threshold to, for example, 80%, then only the fitted dipoles with a residual Deviation of 20% or better are displayed. The results of the other latencies are suppressed in the display.

Mirrored (yz-plane). The Mirrored field forces two mirrored source positions at the yz-plane (midsagittal). If no landmarks are specified, then the mirror-plane normal is parallel to the left-right axis of the original coordinate system (not the PAN system). This constraint cannot be applied when using the Fixed (MUSIC) model.

Add test dipole. The test dipole can be used after a successful fit (e.g., two rotating dipoles) in order to verify the locations. The original results are fixed, and a dipole of the same kind (in this case, a rotating one) is fitted using the adjusted parameters (seed distance, etc.). The test dipole will likely be in the same vicinity as the original ones; if it is far off, then the original solutions may not be valid.

Noise level [μ Vs]. The estimated noise level is computed automatically by averaging the prestimulus interval MGFP values.

4.3.2 Dipole Model Details

The following information will provide a brief introduction to dipole source localization, and describe the different models that may be applied with SOURCE.

A source model is a configuration of generators, which makes sense for the given data. It is the responsibility of the user to choose an adequate source model.

Source models are defined by:

- the number of dipoles,
- the temporal characteristics of the dipoles,
- the dipole locations,
- the dipole orientations, and
- the dipole strengths.

Dipole models are made up of a small number of dipoles, which hardly ever exceeds ten. Each dipole is characterized by six parameters per time point, namely its location and its components.

Single Dipole Models

The simplest dipole model is the *single equivalent current dipole*. Its three location parameters are fitted, and its three components are determined for a given time point so as to minimize the deviation between measured and forward calculated data.

An extension of the single equivalent current dipole is the *moving dipole*. Its three location parameters per time point are fitted, and its three components are determined for each in a series of time points.

If the location of a moving dipole is held fixed over time, we get the *rotating dipole*. Its location is jointly fitted for all time points, while its three components are determined for each time point independently.

A *regional* dipole is a rotating dipole with an additional postprocessing step. A Singular Value Decomposition (SVD) is applied to each rotating dipole in order to determine its preferred orientation and the two other orthogonal components.

If the location and orientation are kept fixed, we have a *fixed dipole*: Location and orientation are jointly fitted for all time points, while for each time point the dipole strength is determined only.

For a *fixed (coh.)* dipole, a common position and orientation for all time points is fitted, and the dipole strengths for every time point are calculated. If more than one dipole is fitted, they will all have coherent loadings (same temporal behavior).

Dipole Constraints

In addition to the requirement that the dipoles to be fitted shall explain the measured data, further requirements can be imposed. These are called constraints, and their purpose is to make the dipole fit more stable and its result more reasonable in certain situations.

SOURCE supports several types of dipole constraints:

- The dipole location does not change over time (rotating dipole).
- The dipole location and orientation do not change over time (fixed dipole).
- The locations of two dipoles are mirrored with respect to the midsagittal plane (*mirrored dipoles*).

Multiple Signal Classification (MUSIC)

Multiple Signal Classification (MUSIC) is a method which does not compute the misfit of a given dipole model per location, but a specific MUSIC metric, with the minimum eigenvalue of the matrix X and the SVDs of the one-dipole lead field matrix L and the spatiotemporal measured data matrix m , respectively.

$$\Delta^2 = \frac{1}{\lambda_{\min}(U^T \tilde{U}_m \tilde{U}_m^T U)}$$

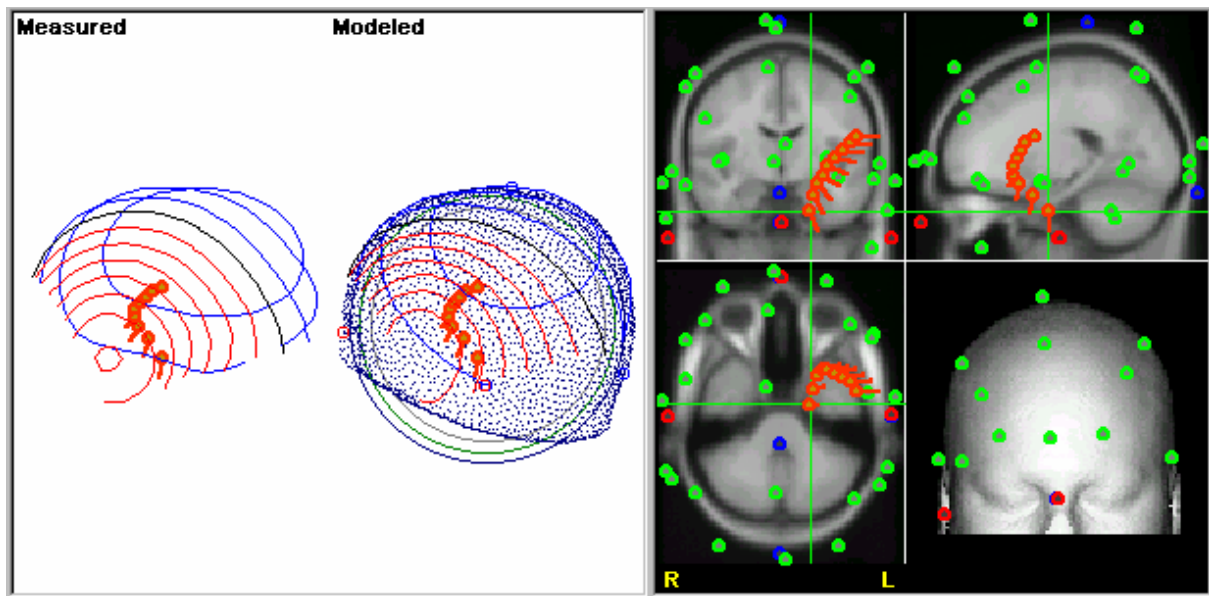
The signal subspace is associated with the leading singular values of U_m standing for the subspace orthogonal to the signal subspace, and associated with the trailing singular values of m . The number of singular values that make up the signal subspace is a parameter of the method.

$$L = U \Sigma V^T \text{ and } m = U_m \Sigma_m V_m^T$$

This metric peaks at the locations of multiple, non-coherent, i.e. temporally independent, sources for a given time range in just a single scan. It gives the best results for temporally independent sources with fixed orientations (e.g., SEPs).

Volume Conductor Models. You have the choice of several volume conductor models to use.

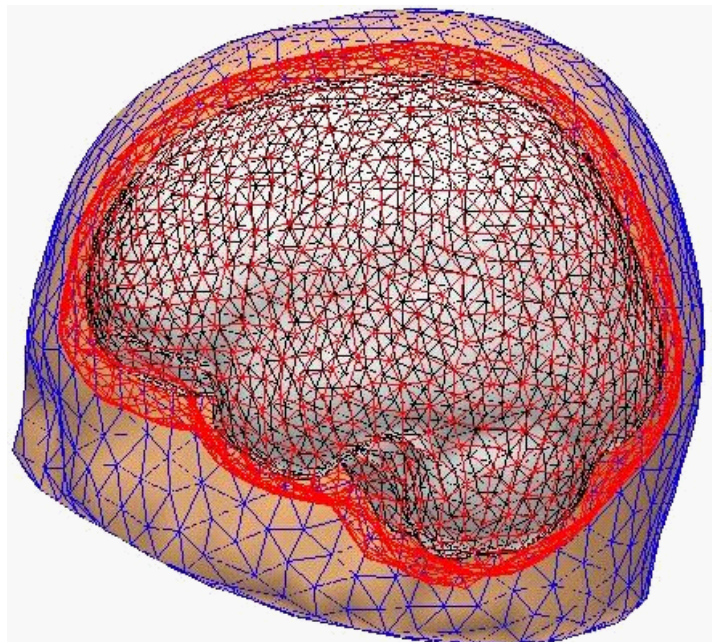
Three Spherical Shells. The three spherical shells volume conductor model parameters are specified in these fields. First, a sphere representing the outermost compartment boundary (skin surface) is fitted to the electrodes, then relative radii as well as conductivity values may be entered. The defaults are standard values from the literature, but you have the option to modify them. You should not scale the volume conductor radii percent values for children or for smaller heads since then the volume conductor would no longer match the electrode positions and the anatomical context of SOURCE. You should see the estimated source positions as rough guesses only and not overinterpret the numerical results. You could scale all numbers offline by the ratio of the measured head circumference to the used value (~55cm, see the log file for numerical details). Especially for small head sizes, however, exactly measured electrode positions are essential. If landmarks are given, the model head surfaces (skin, skull, and brain envelope) are matched to these landmarks.



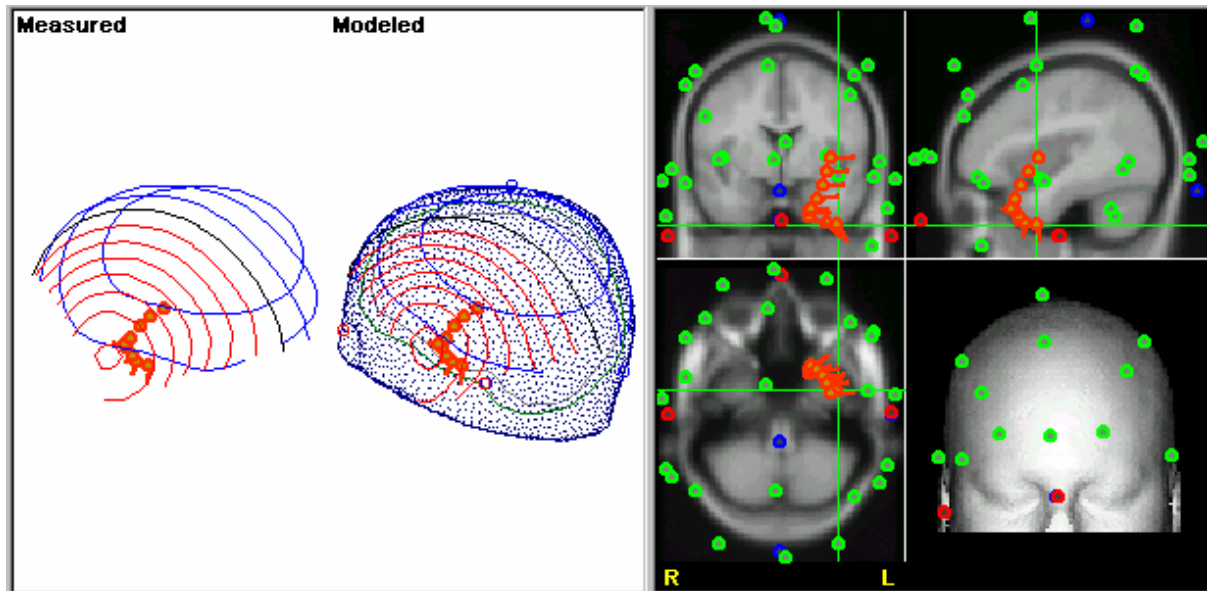
The figure above displays the 5-55ms span of the *EpiSpike.avg* file, using the three spherical shells model.

The BEM and FEM models use the averaged 3D MRI dataset to create three segmented compartments (skin, skull and brain).

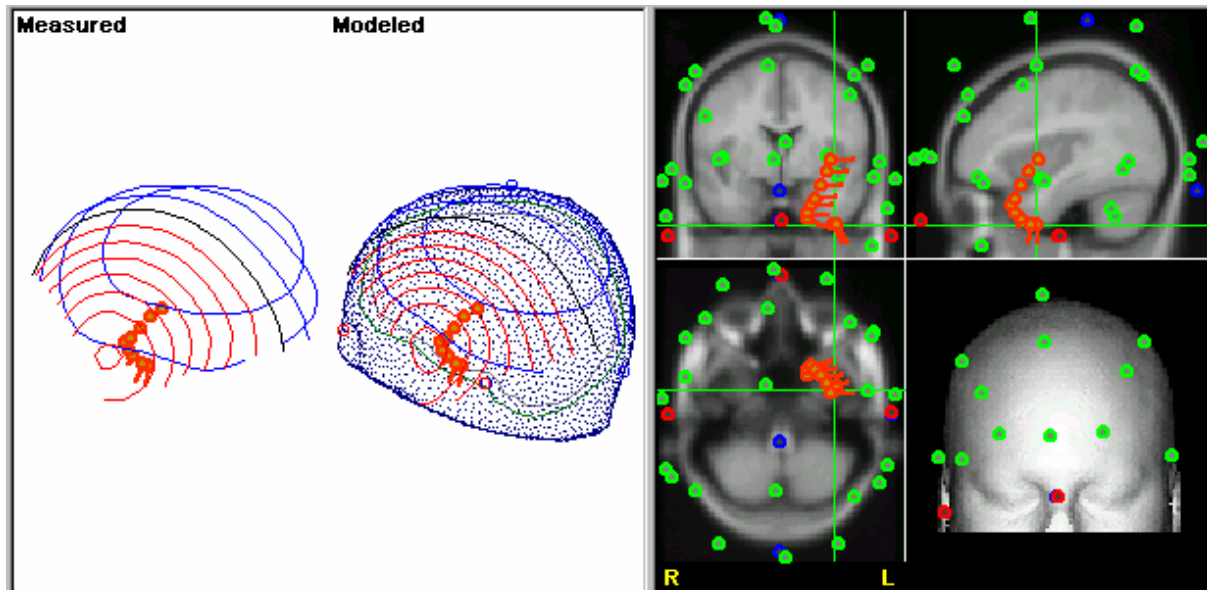
Standard BEM. The standard Boundary Element Model (BEM) consists of 9300 triangles or 4656 nodes, which describe the smoothed cortical envelope (2286 nodes), the outside of the skull (1305 nodes), and the outside of the skin (1065 nodes). The mean triangle edge lengths (node distances) are 6.6, 9.4, and 12.4mm. The triangulated surface appears as follows (image generated from CURRY).



Applying the model to the same interval in the *EpiSpike.avg* file produces the following results.

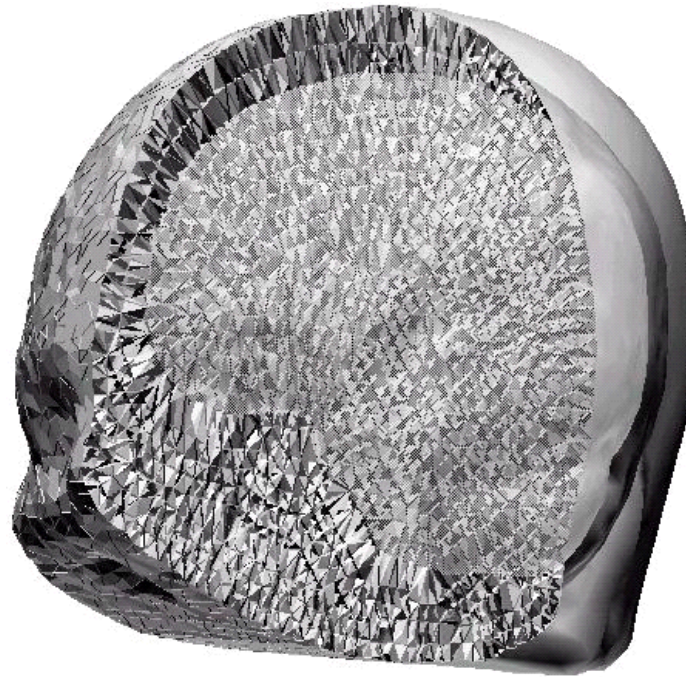


BEM interpolated. The interpolated BEM model consists of 8043 nodes (brain: 3858, skull: 2681, and skin: 1504 nodes). The mean triangle edge lengths 5.1, 6.6, and 10.4mm. The stepsize of the 3D grid of the precomputed leadfield matrix is 5mm. The linear interpolation of the lead field is very similar to the one described in B. Yvert, et. al., Human Brain Mapping, 14, 48-63, 2001.

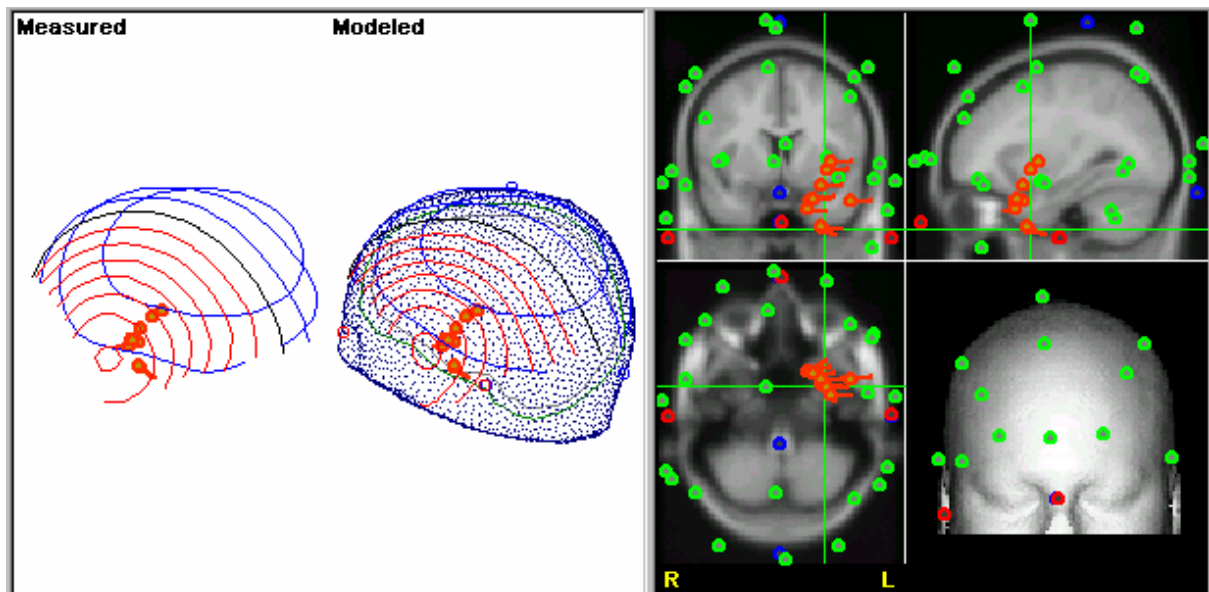


FEM interpolated. The Finite Element Model (FEM) represents the surface using 286,000 tetrahedra, with an edge length of 4mm. The stepsize of the 3D grid of the precomputed leadfield matrix is 6mm. Interpolation is the same as for the BEM interpolated model. The tetrahedral surfaces appear as follows

(image generated from CURRY).



Applying the FEM model to the same span in the *EpiSpike.avg* file produces the following results.



Display Options. If the automatic coordinate system orientation detection fails, it can be overwritten using the x y z, y z x, or z y x options (referring to the order of the coordinate system axes in the electrode positions file, where x means right - left, y means anterior - posterior, and z means bottom - top).

Contour incr [μV]. The Contour setting is used to determine the increment

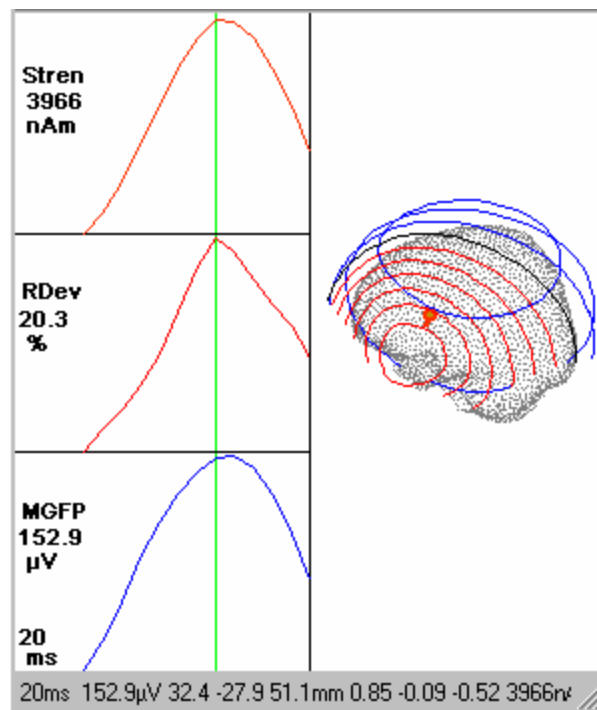
between the contour lines. For example, if set to $0.5\mu\text{Vs}$, the contour lines will be drawn for each $0.5\mu\text{V}$ interval. You may also use the up and down arrows from the keyboard to change the contour interval in the SOURCE display.

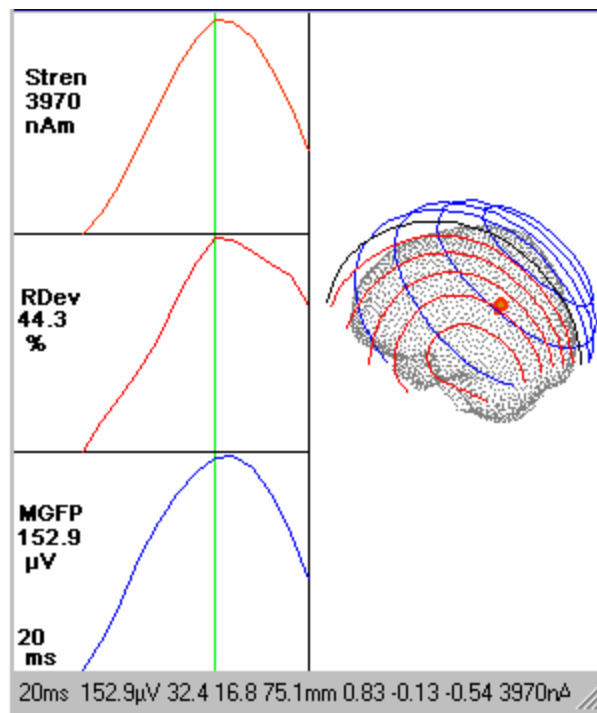
Movie/rotation delay [ms]. The Movie/rotation delay time [ms] (0...1000ms) determines the replay speed for AVI movies (and also in the saved movies as well). The smaller the number, the faster the replay time (the number is the number of ms each frame is displayed). Saved AVI movies can also be replayed with Microsoft's Media Player (and edited by JASC's PaintShop Pro, see www.jasc.com).

4.3.3 Hypothesis testing

If you get a dipole result in the vicinity of the "true" location that you expect from your paradigm, you can easily move the dipole position to the expected location (grab and drag it in a plane parallel to the "screen" plane), and see how well the data could be explained with a source at the "right" spot. (You will see the Source Waveform and Deviation % vary with the new position). Often the error hyperfunction has a very shallow 'sink' (especially if you try to analyze data with a low SNR: if you double the SNR, the confidence radius of the found solution reduces to one half), and there is only a slightly better fitting position found (e.g. 9.8% residual deviation) by the minimization algorithm as compared to the "correct" position (e.g. 9.9% residual deviation).

The figures below show the original location (left), and the repositioned location (right).





4.4 The Option Menu for SLICE

The Option Menu for SLICE. Click the right mouse button within the SLICE display and you will see the following list of options. Some of these are the same as those described above in the SOURCE options. The new ones are described below.

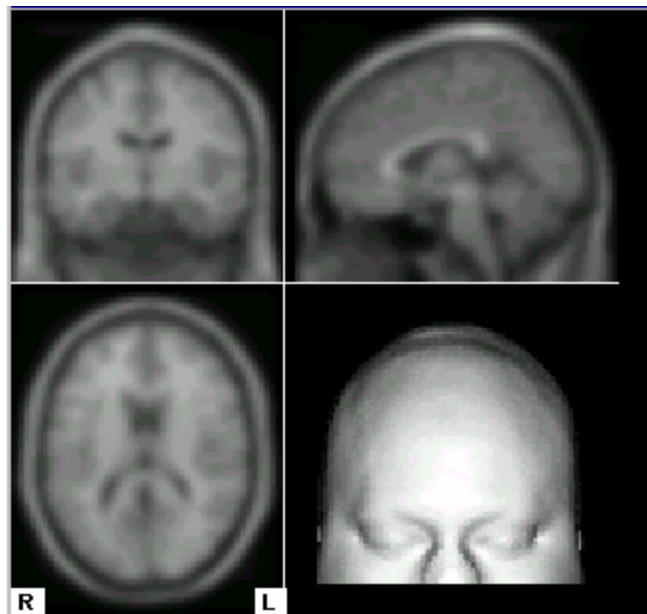
Display	►
View	►
Set Reference	R
Show Reference	Alt+S
Set Nasion	Ctrl+N
Set LPA	Ctrl+L
Set RPA	Ctrl+R
Set Vertex	Ctrl+T
Set Inion	Ctrl+I
Get Position	G
Delete Position	X
Delete All Positions	Ctrl+D
Copy to Clipboard	Ctrl+C
Save As (*.bmp, *.emf)...	Ctrl+A
Help...	F1
Select Data...	S
Data Parameters...	P

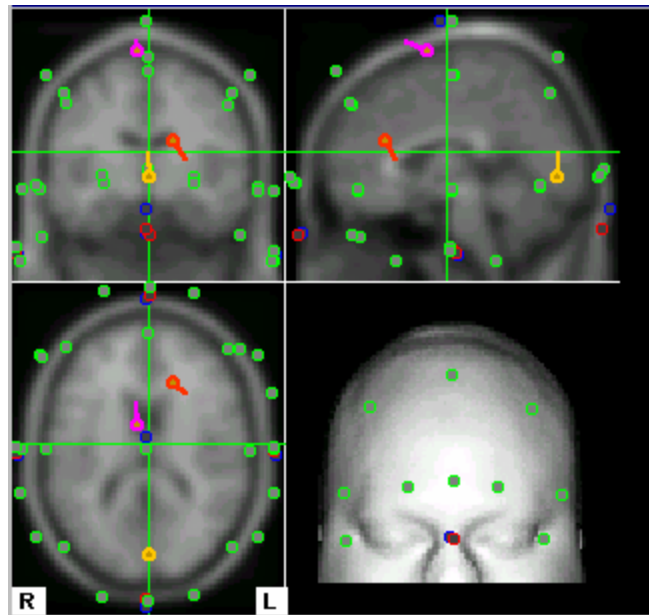
Display. The Display options let you select the elements you wish to include in the

SLICE display. The Crosshair, Dipoles, Electrodes, Landmarks and Confidence Ellipsoids may be toggled on or off.

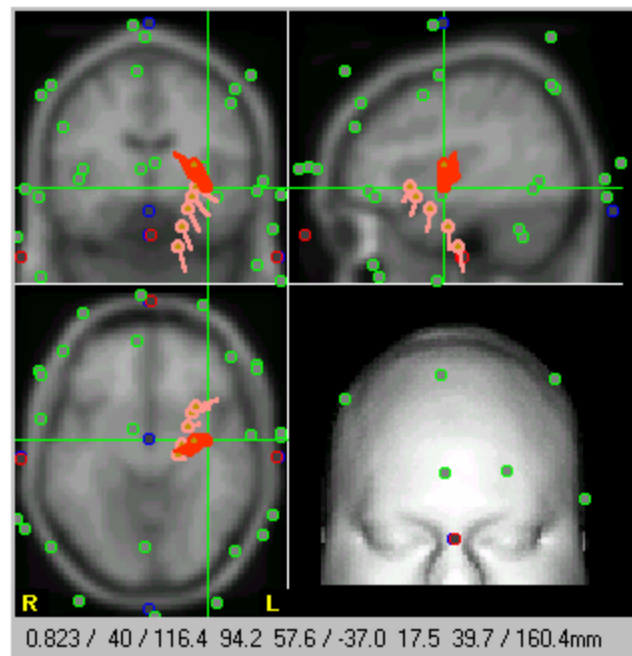
✓ Crosshair	C
✓ Dipoles	D
✓ Electrodes	E
✓ Landmarks	L
<hr/>	
✓ Conf. Ellipsoids	Alt+C
<hr/>	
Keep Results	Alt+K
Reset Results	Alt+X
<hr/>	
Maximum IP	M
Reset Grayscale	Alt+G

The figures below show how the SLICE display will appear with all of the options off and on.

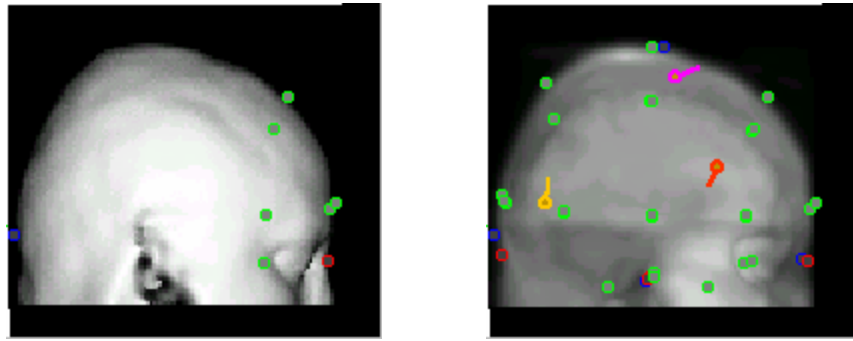




Keep Results / Reset Results. The Keep Results option retains the latest dipole solution on the display while you compute new results (new mode, latency, interval, etc.) on the same display. The "kept" results are shown in pink, and the new results are shown in red. Clicking Reset Results will remove the kept results.



Maximum IP. The Maximum IP (Maximum Intensity Projection) option affects the image in the rendered view (lower right corner of the SLICE display). The figures below show the image (right side view) with Maximum IP disabled, and then enabled.



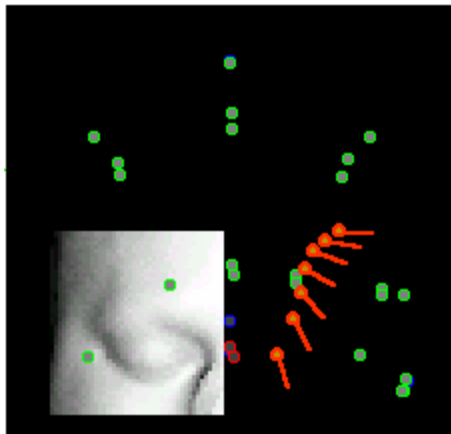
Reset Grayscale. In Maximum IP mode, you can vary the intensity of the white end and the black end of the grayscale by rotating the mouse wheel (white), and by holding the Shift key down while rotating the mouse wheel (black). Use the Reset Grayscale option to return to the default settings.

View. The View option lets you select the viewing perspective of the rendered head (the one in the lower right hand corner of the SLICE display). The Cut options allow you to cut out parts of the rendered view, and the Scale options let you quickly change the size of the SLICE display. These options are discussed in more detail below.

✓ Frontal View	Alt+F
Left View	Alt+L
Right View	Alt+R
Top View	Alt+T
Back View	Alt+V
Bottom View	Alt+B
<hr/>	
Cut Left	Alt+E
Cut Right	Alt+I
Cut Bottom	Alt+O
Cut Top	Alt+P
<hr/>	
Scale = 1.0	Alt+1
Scale = 2.0	Alt+2

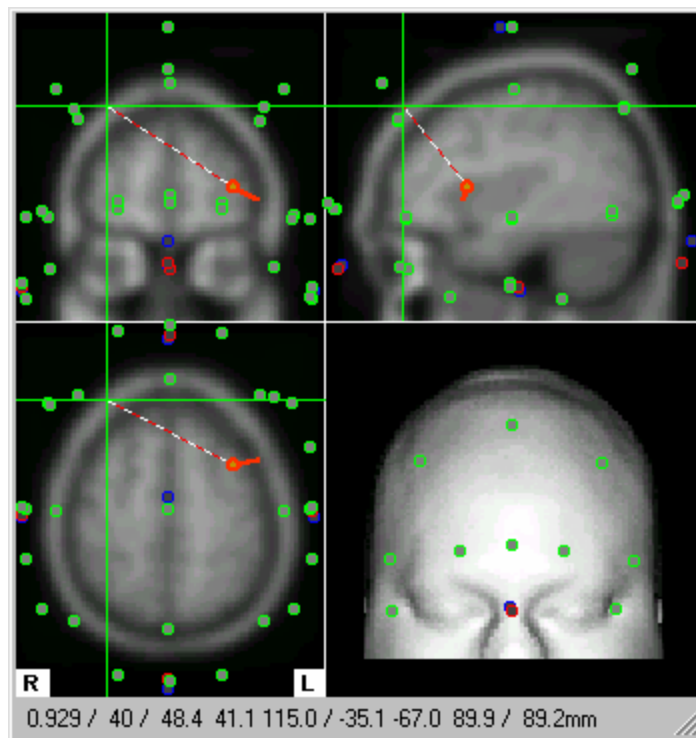
Frontal to Bottom Views. The various views will change the viewing perspective for the rendered and the Maximum IP views.

Cut sections. The Cut options let you selectively cut out parts of the rendered view. Cut Left (Right) cuts out the left (right) side of the head. Cut Bottom (Top) cuts the bottom (top) half of the head. You can combine options like Cut Left and Cut Top to display only the lower right quadrant.



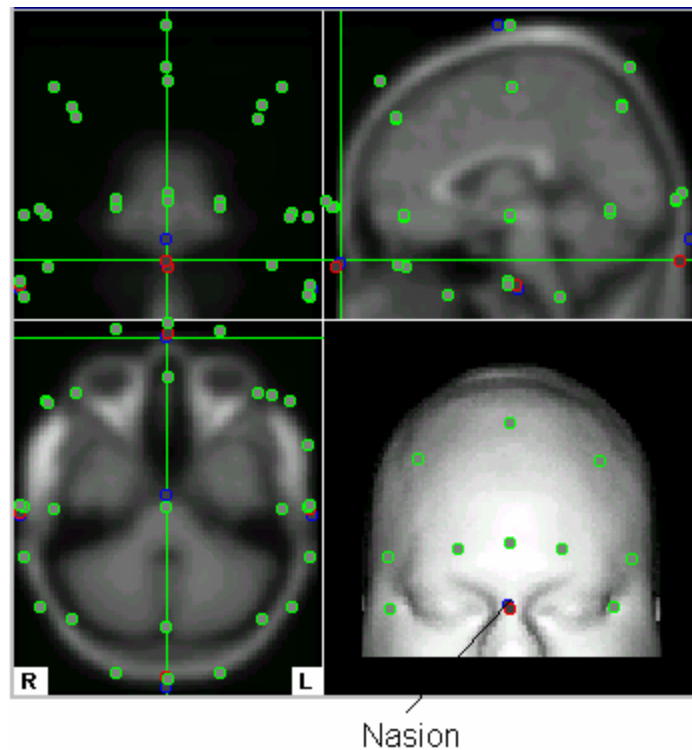
Scale = 1.0 / Scale = 2.0. These options provide a quick means for changing the size of the SLICE display (Scale = 1.0 is the small size; Scale = 2.0 is the large size; units: display pixels / mm).

Set Reference/Show Reference. These two features are used to measure physical distances in the image (and have nothing to do with the Reference electrode). In this example, we are using a single fixed dipole, and we want to measure the distance between its location and the skin surface. Position the crosshairs on the dipole source (if they are not already there). Right click inside the SLICE display, and select Set Reference. This sets that point as the Reference point for measurement. Then right click again, and select Show Reference. Now as you move the crosshairs around you will see the measurement line, going from the current position to the reference point. Measured distances are displayed at the bottom of the display on the Status bar
0.929 / 40 / 48.4 41.1 115.0 / -35.1 -67.0 89.9 / 89.2mm . The last number is the distance (in mm) between the Reference point and the cursor position.

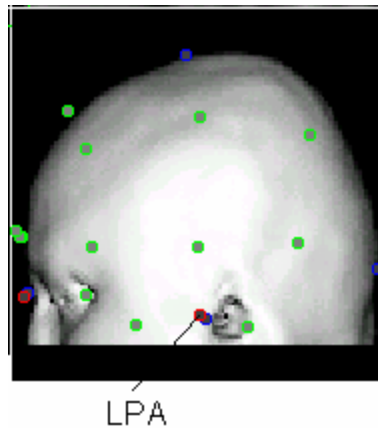


Set Nasion through Set Inion. These options must be used when you are importing your own MR or CT data to indicate the locations of the landmarks.

To set the Nasion, position the mouse cursor at the nasion on the rendered surface, and click the left mouse button.



(In this example, the nasion has already been registered). Then click the right mouse button, and select the Set Nasion option, or, use the *Ctrl+n* combination keystrokes. Change the view of the rendered surface to Left View, and select the left preauricular point, using the same procedure.

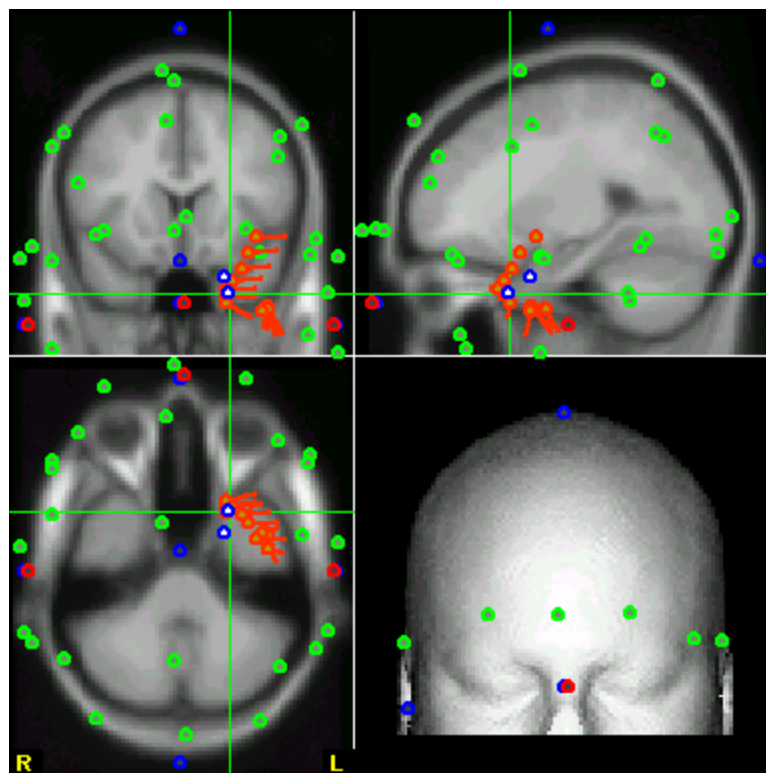


Repeat the process to register all 5 landmarks.

Get Position, Delete Position, Delete All Positions. The Get Position option is used to mark points within the SLICE display. The points are marked with a blue/white circle.

Get Position	G
Delete Position	X
Delete All Positions	Ctrl+D

The position data are saved using the Save Marker Positions As option (right mouse menu option accessed from the SOURCE display). The position data are saved in an ASCII text file (having a .dig extension).

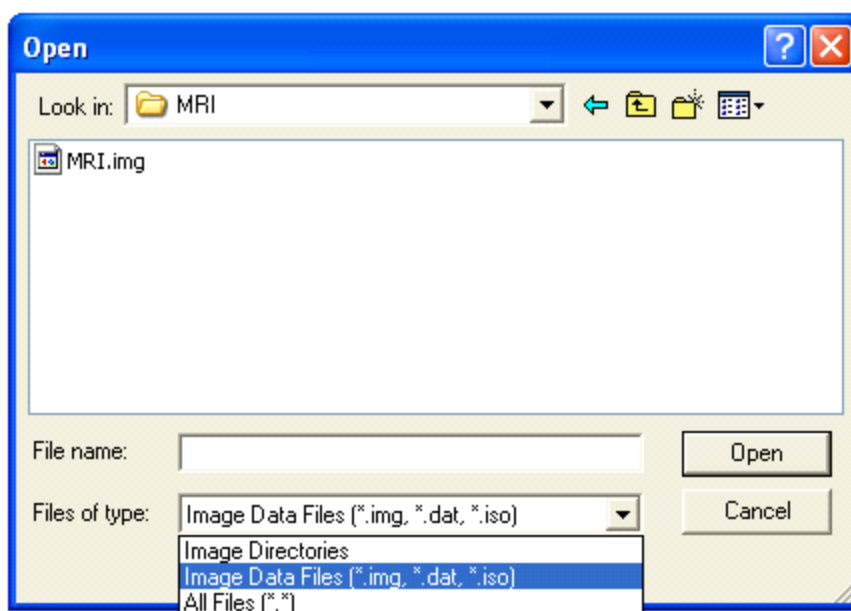


Delete Position is used to remove the most recently marker position; Delete All Positions deletes all marked positions.

Miscellaneous options. These include *Copy to Clipboard* and *Save As (*.bmp, *.emf)*, and are the same as described above under the SOURCE *right mouse* options description. The *Help* option displays the SLICE Help screen (also described above).

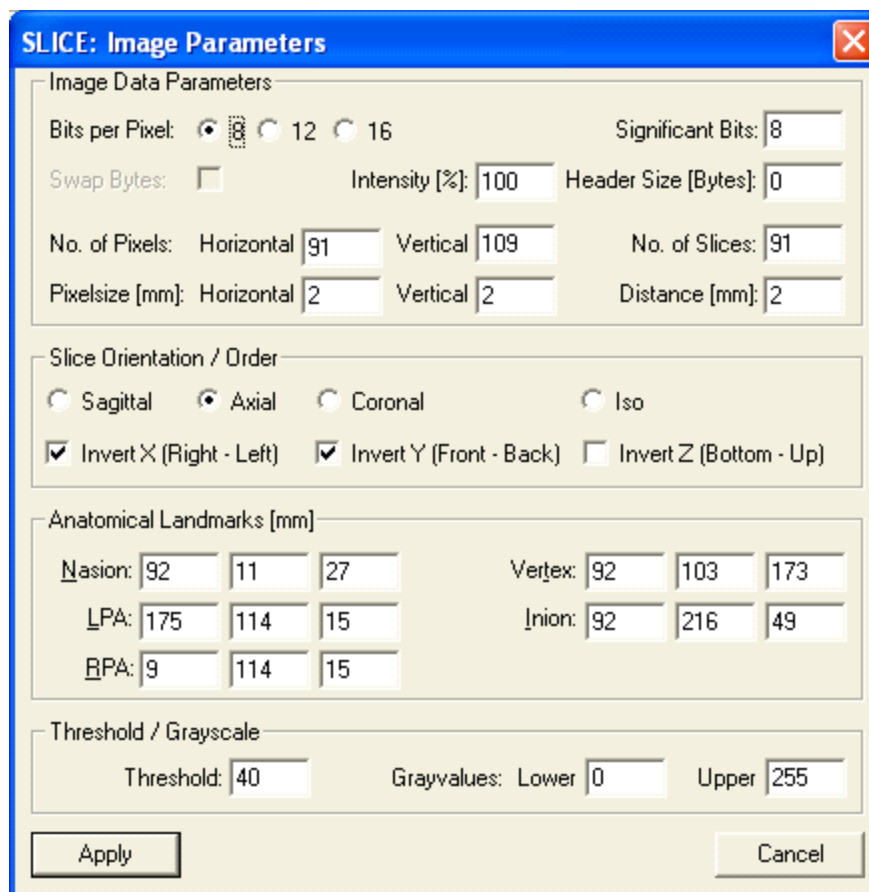
Copy to Clipboard	Ctrl+C
Save As (*.bmp, *.emf)...	Ctrl+A
Help...	F1

Select Data. The Select Data option allows you to import other MR files. The standard Open File utility window will let you select IMG, DAT or ISO data files. You also have the option to load image data that are saved in separate image files by specifying the directory that contains the slices (and *only* the slices).



The Data Parameters display will appear.

Data Parameters. Clicking this option displays the Image Parameters window.



If you are using the internal (warped) MRI data set that is compiled into the SLICE program, these fields cannot be modified. You will see an error message on the bottom of the SLICE window, after pressing the "Apply", button, saying

cannot overwrite internal data parameters ! parameters can be edited / stored for external image data only

The Image Parameters window displays the set parameters and allows you to edit them if you read in real MR or CT data. If you try to read an image data set for the first time (where no parameters have been set), you will see the Image Parameters window and you will need to fill in the information that is necessary to read the data correctly. After pressing "Apply", the parameters file will be written (.imp - image parameters) and the image data will be read (.dat, .img, .iso) and displayed.

In order to coregister with the EEG sensors and reconstruction results, the five landmarks have to be set (the actual cursor position will be taken and the coordinates will be transferred to the parameters window; see "Set Nasion through Set Inion" above). When all five landmarks are set and 'Apply' is pressed, the .imp-file will be overwritten, the image data will be reloaded, and are now ready to display electrodes and reconstruction results from SOURCE.

Image Data Parameters. This section of the display contains descriptive information about the raw data (2D slices).

Bits per Pixels. Image data can be stored with one byte (8 bits), one and a half bytes (12 bits), or two bytes (16 bits) per pixel. Each pixel contains the gray level information of one 2D image point (pixel).

Significant Bits. Within the 8, 12, or 16 bits per pixel, not all bits may be used (sometimes only 8 or 12 of 16 bits are actually used). This can be accounted for by this setting. Typically, 12 of the 16 bits are used to store the image. If you see a rather dark image, try decreasing the number of Significant Bits (such as from 12 to 9).

Intensity. The image intensity can be scaled in powers of 2 (bit-wise) or continuously using the Intensity field. The grayscale can be inverted by using negative numbers (e.g., -100%).

Swap Bytes. Image data can be stored in MOTOROLA or INTEL byte order, depending on the raw data processing machine. Byte order can be toggled by this setting. If you have not enabled Swap Bytes, and after clicking Apply you see a noisy image, try enabling Swap Bytes and then press Apply again.

Offset (Header Size) [Bytes]. Each slice of the image data often contains a header of a defined size (e.g. ACR-NEMA data). The set number of bytes will be skipped. The size of the header can in most cases be calculated from the file size S , where the size of one slice $s = S / \text{No_of_Slices}$ [Bytes]. Header size (per slice) $H = s - (\text{No_of_Horizontal_Pixels} * \text{No_of_Vertical_Pixels} * \text{Bits_per_Pixel} / 8)$.

For example, say a slice is 152,244 bytes (use the file properties to get this value). This means that with the typical image size of 256x256 pixels, there are 2 bytes (16 bits) per pixel ($256 \times 256 \times 2 = 131,072$ bytes) plus a header of $152,244 - 131,072 = 21,172$ bytes.

There are two ways to read the data:

- 1) Read the data from the front of the file where there is an offset of 21, 172 bytes (header) for each slice (the offsets have to be equal for all slices) - in that case the Header Size [Bytes] is 21,172.
- 2) Read the data from the end of each slice (in which case the offset can be variable) - in that case the Header Size [Bytes] is -1.

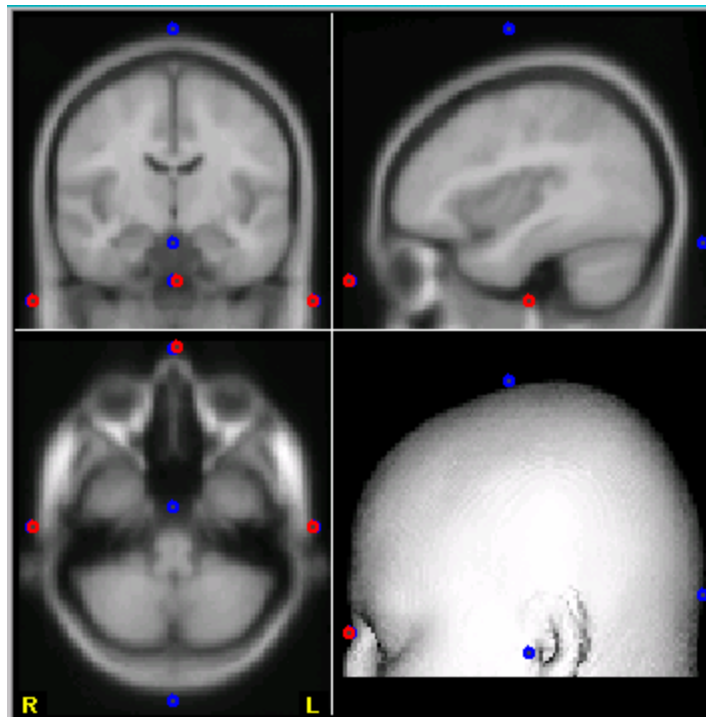
The remaining fields are fairly self-explanatory, and display the number of pixels in the horizontal and vertical axes (typically 256), the horizontal and vertical pixel size (in mm's; use 1mm if you are unsure), the total number of slices, and the distance (thickness).

Slice Orientation / Order. These fields describe the sequence and orientation of the 2D raw data slices in their 3D context, and are for the most part self-explanatory. "Iso" is the 8_Bits_per_Pixels isotropic data format Curry can generate and dump to disk. Special care should be taken with the Invert X (Right - Left) checkbox, since without an image marker this can erroneously result in a left-right reversal (the effect of the other checkboxes shows up immediately).

Anatomical Landmarks [mm]. Anatomical Landmarks are needed for coregistration of the anatomical image data with the functional data (EEG). The five landmarks have to be set by using the Set Nasion through Set Inion items (described above) on the SLICE options menu (click the right mouse inside the SLICE window, or use the keyboard combination strokes). The actual cursor position will be taken and the coordinates will be transferred to the parameters window. When all five landmarks are set and "Apply" is pressed, the .imp-file will be overwritten and the image data will be reloaded. You are now ready to display the results in SOURCE.

You may notice that some landmarks appear in red and others are in blue.

The anatomical landmarks (blue, in this example) in SOURCE are predefined and fixed for the averaged MRI dataset that was used to segment the point clouds (skin, skull, and brain). These segmented compartments are also used to set up and precompute the BEM/FEM models. Thus, these landmarks have to be fixed and cannot be edited.




The corresponding functional landmark positions (red, in this example) have to be measured together with electrode positions using a 3D digitizer (e.g. Polhemus). They are used to register the real electrode positions to the averaged MRI model coordinate system.

If an individual anatomical data set is used to overlay it with electrode positions and reconstruction results, the corresponding anatomical landmark positions have to be defined in SLICE. So these landmarks are needed to transform the (functional) electrode / landmark positions and reconstruction results for display purposes only. These landmarks are also used to construct the PAN coordinate system within the individual anatomical dataset.

These individual anatomical landmarks are NOT used in SOURCE. SOURCE always uses the averaged MRI with its predefined landmarks for BEM reconstructions and overlay (point clouds).

If label matching is performed in SOURCE, the predefined averaged MRI landmark and predefined electrode positions are used.

Threshold / Grayscale. The Threshold / Grayscale parameters are the initial settings for the surface rendering and graylevel scaling of the MR / CT images. These can also be modified interactively by the mouse wheel (with and without the Shift key).


The  button saves the settings to the .imp-file (image parameters) and reloads the image data using these parameters.

Note: You may select or vary any of the options in the SLICE Image Parameters display, and see the effects by clicking Apply, without closing the Parameters

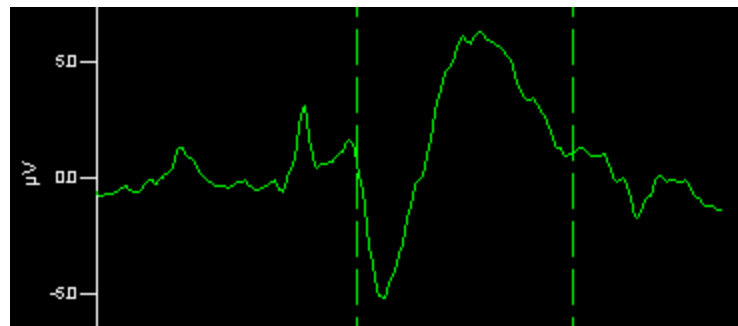
window. The Options menu (right mouse button) will remain accessible while the SLICE Parameters display is seen.

4.5 Online SOURCE

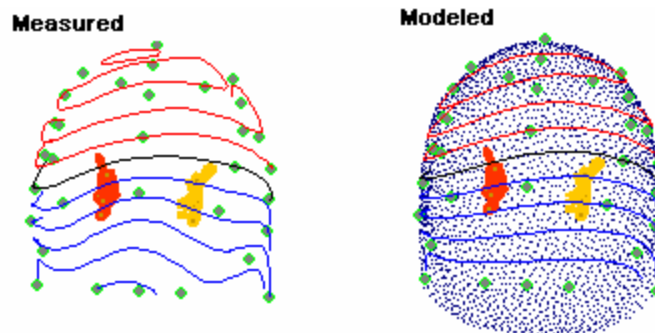
The information above has described the functions of SOURCE in offline processing. It is also possible to use most of the same features during online acquisition. SOURCE can be used with any online Multiple Window Display, such as online averages or sorted averages. There is currently no online application of SOURCE for continuous acquisition, and Tracking

mode is not available online. Once acquisition has begun, click the  icon from the Toolbar. Make sure the desired window has the focus. Then set the analysis interval, and the functions are the same online as they are offline.

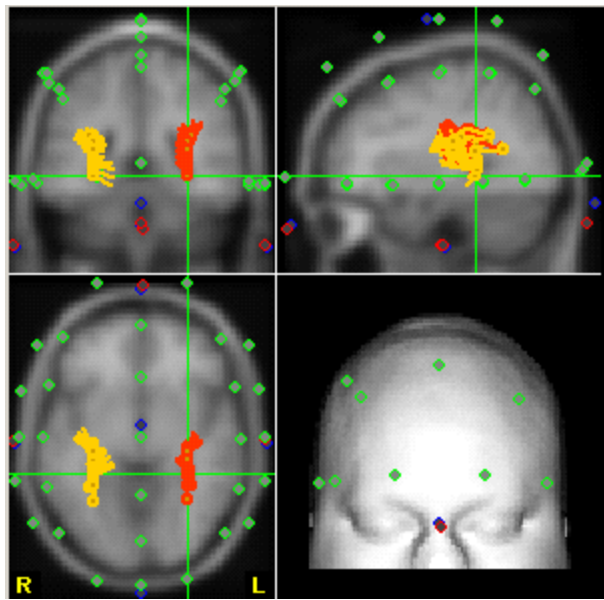
For an illustration, we collected online binaural AEPs and computed the moving dipole solutions. The waveforms after 100 sweeps appeared as follows.



The SOURCE solution for the approximate 110-260ms span appeared as:



and the SLICE display appeared as shown.



The dipole solutions were apparent early in the recording (after about 14 sweeps) - coincident with the appearance of the components in the online average.

5 Suggested REFERENCES for more information

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M. Fuchs, R. Drenckhahn, H.-A. Wischmann, M. Wagner, "An Improved Boundary Element Model for Realistic Volume Conductor Modeling," *IEEE Biomed. Eng.*, Vol. 45, No. 8, pp 980-997, 1998

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M. Fuchs, M. Wagner, J. Kastner, Boundary Element Method Volume Conductor Models for EEG Source Reconstruction, *Clinical Neurophysiology*, 2001, 112: 1400-1407

B. Yvert, A. Crouzeix-Cheylus, J. Pernier. Fast realistic modeling in bioelectro-magnetism using lead-field interpolation, *Human Brain Mapping*, 2001, 14: 48-63

M. Fuchs, J. Kastner, M. Wagner, S. Hawes, J.S. Ebersole, A Standardized Boundary Element Method Volume Conductor Model, *Clinical Neurophysiology*, 2002

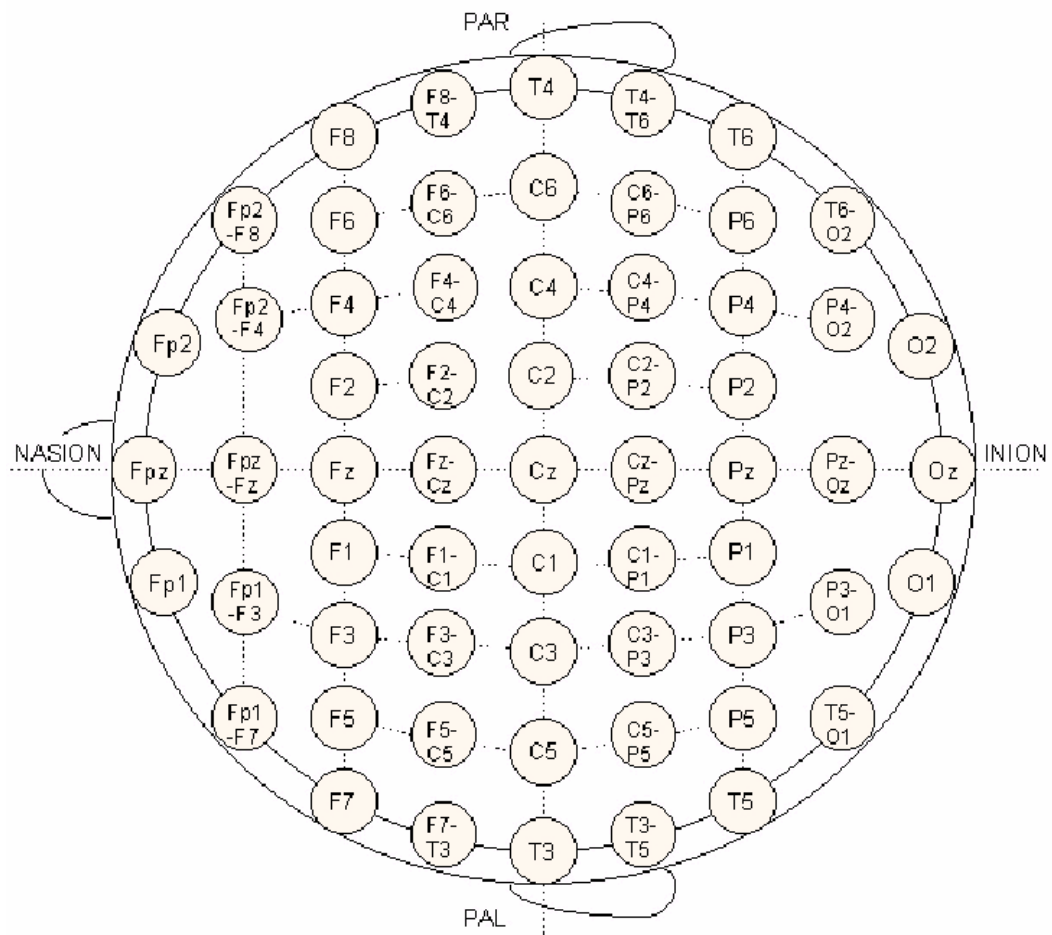
6 Appendix A - Label Matching

SOURCE uses a label matching algorithm to retrieve the electrode positions (positions of the 10/20 system) by their labels, if no actual 3D positions are given or available. All electrodes with a matching label (see list below) will be used in the source reconstruction (non-matching ones will be excluded).

Each line contains up to four equivalent electrode labels for a known electrode position. Where there is a single label on a line, no equivalent labels are recognized. (Numbers 41-46 are not used in source reconstruction).

1	TP10	T10-P10			47	O9			88	P1
2	TP9	T9-P9			48	O10			89	P2
3	TP11	T11-P11	A1		49	CB1			90	P6
4	TP12	T12-P12	A2		50	CB2			91	C5
5	FT11	F11-T11			51	SP1			92	C1
6	FT10	F10-T10			52	SP2			93	C2
7	FT12	F12-T12			53	Fp1	FP1		94	C6
8	FT9	F9-T9			54	Fp2	FP2		95	F5
9	AF7	FP1-F7	Fp1-F7		55	Fpz	FPZ		96	F1
10	AF3	FP1-F3	Fp1-F3		56	F11			97	F2
11	AFz	AFZ	FPZ-FZ	Fpz-Fz	57	F10			98	F6
12	AF4	FP2-F4	Fp2-F4		58	F12			99	F9
13	AF8	FP2-F8	Fp2-F8		59	T10			100	T9
14	FT7	F7-T3	F7-T7		60	T11	MN1		101	P9
15	FC5	F5-C5			61	T12	MN2		102	M1
16	FC3	F3-C3			62	P10			103	M2
17	FC1	F1-C1			63	P11			104	A1
18	FCz	FCZ	FZ-CZ	Fz-Cz	64	P12			105	A2
19	FC2	F2-C2			65	Pal	PAL	LPA	106	T1
20	FC4	F4-C4			66	Par	PAR	RPA	107	T2
21	FC6	F6-C6			67	Iz	IZ	INI		
22	FT8	F8-T4	F8-T8		68	Nz	NZ	NAS	Ini	Nas
23	TP7	T3-T5	T7-P7		69	O1				
24	CP5	C5-P5			70	O2				
25	CP3	C3-P3			71	P7	T5			
26	CP1	C1-P1			72	P3				
27	CPz	CPZ	CZ-PZ	Cz-Pz	73	Pz	PZ			
28	CP2	C2-P2			74	P4				
29	CP4	C4-P4			75	P8	T6			
30	CP6	C6-P6			76	T7	T3			
31	TP8	T4-T6	T8-P8		77	C3				
32	PO7	T5-O1	P7-O1		78	Cz	CZ			
33	PO3	P3-O1			79	C4				
34	POz	POZ	PZ-OZ	Pz-Oz	80	T8	T4			
35	PO4	P4-O2			81	F7				
36	PO8	T6-O2	P8-O2		82	F3				
37	PO5				83	Fz	FZ			
38	PO9				84	F4				
39	PO10				85	F8				
40	PO6				86	Oz	OZ			
xxx	41	IO1	xxx		87	P5				
xxx	42	IO2	xxx							
xxx	43	SO1	xxx	not used for						
xxx	44	SO2	xxx	reconstruction						
xxx	45	LO1	xxx							
xxx	46	LO2	xxx							

The standard 10-20 system electrode positions are shown below. Note that some labels in the figure should be replaced with newer labels. For example, T3 is now T7, T4 is now T8, T5 is now P7, T6 is now P8, and so forth.



An interesting paper about the 10/20 system and the electrode labels is:

G.E. Chatrian, E. Lettich, P.L. Nelson, "Ten Percent Electrode System for Topographic Studies of Spontaneous and Evoked EEG Activities", *Am. J. EEG Technol.* 25, 83-92, 1985.

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