Visual Photons

Formation and Sensation of Retinal Images

author: Jonathan D. Lettvin written: Apr 01 2015 fetched: Apr 27 2015

1 Introduction

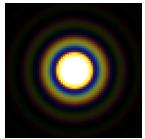


figure 1: Airy pattern

Whither and whence visual photons needs must uncertain be yet by lawful pattern ruled. Photons are produced, scattered, reflected, refracted, diffracted and, finally, incident and aborbed by the retina in "bleaching" events. Daylight photons result from solar blackbody emissions with notches due to atmospheric absorption. Surviving photons are scattered by the atmosphere, reflect off objects, refract through the cornea, diffract through the pupil, and are absorbed by various species of photoreceptors. Each of these processes contribute to spectral transforms.

In the study of perception, there appear to be laws governing invariance. Contrast invariance and color invariance are two popular study subjects. It is not possible to discuss these invariants without discussing the quantitative absorption of photons by the retina from a typical scene. Most modern synthesis of images depends on the use of RGB emission usually produced by LEDs and for purposes of improving robotic vision. Notwithstanding the LMS

retinal cone species having similar spectral peaks, the images produced for use with an achromatic lens and with an Airy disk smaller than a pixel for a digital camera are not suitable for analyzing images produced by the chromatic natural lens and Airy disk always larger than the human equivalent of pixel. The subject of this paper is the production ane encoding of synthetic images suitable for analysis of human visual invariants.

Two transforms dominate the formation of images on the retina; corneal refraction and pupillary diffraction. Both have λ (wavelength) dependence. Corneal refraction is modelled by a $1/\lambda$ proportional affine transform where short wavelengths are expanded more than long wavelengths. Pupillary diffraction is modelled by convolution with a λ proportional Airy kernel; where the kernel is smaller for short wavelengths and larger for long wavelengths. In other words, for a white object on a black background you will oberve a blue tinge ringing the object as seen through a magnifying glass and a red tinge ringing it as seen in the Airy disk from a pinhole.

Both of these transforms apply to mathematical models of images formed from photons counting in the millions or billions. The affine transform from refraction is modelled simply enough. Analysis of diffraction and synthesis of suitable diffraction images from very low to very high photon counts will be the primary focus of this paper. Images produced and encoded using these methods will enable further research into how retinal processing achieves invariance.

Point Source Diffraction

When a very large number of photons from a point source pass through an aperture and then fall on a surface they accumulate in a diffraction pattern called an Airy pattern figure¹. This intensity pattern is the square of the photon wave function equation⁶. Photon densities are properly synthesized by summing the wave equations for all points over all wavelengths and squaring the result.

This pattern of intensity is ruled by equation⁴. This formula represents the idealized continuous distribution from which deviation is unmeasurable at high photon counts. Discrete photons do not form a continuous set. Nor do sensors arranged along a grid in a focal plane in an eye or camera. The zoomed "pixels" in figure ¹ illustrate this grid for billions of RGB source photons seen for a centrally located point source.

Close examination reveals that different wavelengths contribute differentially to the pattern at different radii. Photographic and visual colors are typically thought to operate using RGB. The names R (red), G (green), and B (blue), as wavelengths, are typically thought to be related to color perception. In fact, color perception is independent of wavelength Lettvin et al¹. The scientific labelling for RGB in retinal photoreceptor absorption is LMS for Long, Medium, and Short. However, since photography and displays use RGB, they will be used interchangeably.

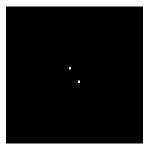


figure 2: 2 white points

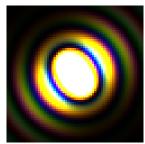
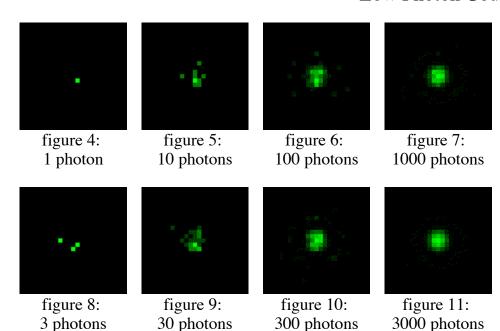


figure 3: Retinal image with a 1mm pupil

The retinal image of two white RGB point sources incident on the human retina after traversing a 1mm pupil appears as an inchoate blur incapable of being resolved by Rayleigh criterion, Sparrow limit, or even traditional use of Fourier transform coupled with Nyquist sampling.

The wavelength dependence in figure³ is even more apparent than for figure¹. This is the character of image for narrow band RGB illumination. This paper will explore the problem of forming retinal equivalent incident photons using broadband illumination and methods for producing suitable sensed images for analyzing how the sensory data for vision is presented. Even in figure³, enough photons are present to give the image a seemingly continuous character.

Low Photon Count Diffraction



When photon flux is low, the Airy pattern becomes more difficult to discern as can be seen in the models of accumulations of single monochromatic photon events in figure⁴ to figure¹¹.

As can be seen, even at 3000 photons from a point source the Airy pattern is yet to assume the continuous character achieved at much higher photon fluxes experienced in daylight or even low incandescent lighting.

Vision still works fairly well at low light levels so whatever explanation is made for vision must account for the ability to convert patterns such as these to good enough quality internal reconstructions of the scene.

It is important to note that, when point sources are eccentric from the center, different wavelength photons refract and diffract to different centers aligned radially from the center; yet the perception of a polychromatic point is of a single point source.

Photons, Spectra, and Blackbodies

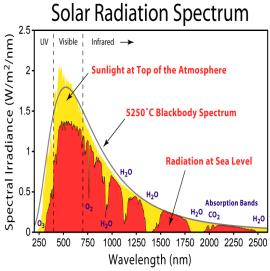


figure 12: Solar Spectrum (wikimedia commons)

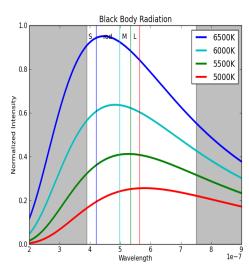


figure 13: Blackbody radiation (visible wavelengths are within the white region of the figure. The peak absorption of typical human photoreceptors are shown as colored vertical lines)

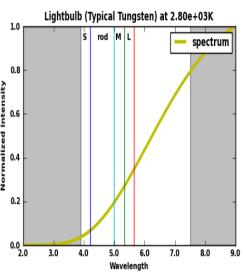


figure 14: Light bulb (at a lower blackbody temperature of 2800K, longer wavelengths dominate unlike sunlight where shorter wavelengths dominate)

Natural lighting is not divided into photons having 3 or 4 energy bands discussed in robotic vision literature. **Daylight** spectra are considered continuous in that no energies or wavelengths are forbidden. Typically, ambient light

is broad spectrum as in figure ¹³. Sunlight resembles the 6500K curve with atmospheric absorption. An incandescent lightbulb peak temperature is 3695K which yields a slope that appears to rise monotonically from the blue end to the red end. The spectrum of figure ¹⁴ is typical for a light bulb at 2800K. When moving from sunlight into incandescent light one does not perceive a change in colors. The change of spectrum does not change the colors seen but the size, shape, and spectral composition have changed dramatically by the change in light source.

The two spectra of figure ¹³ and figure ¹⁴ were produced with equation ². The theory of this curve is well explored. Blackbody radiation may be specified with two parameters, T (degrees Kelvin), and visual angle (or amplitude).

$$I(\lambda, T) = \frac{2hc^3}{\lambda^5} \frac{1}{exp(\frac{hc}{\lambda kT}) - 1}$$

Blackbody equation in λ [1]

$$I(\nu, T) = \frac{2h\nu^3}{c^2} \frac{1}{exp(\frac{h\nu}{kT}) - 1}$$

Blackbody equation in ν [2]

where:

 $h = Planck\ constant$

c = speed of light in a vacuum

k = Boltzmann constant

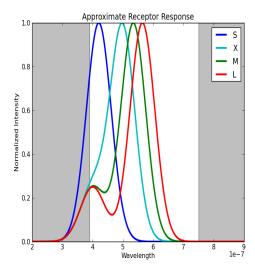
 $\nu = photon\ frequency$

T = body temperature in Kelvin

Other spectra like figure ¹⁵ and figure ¹⁶ are generated using short lists of coefficient triples (a,b,c). The curves in both of these figures took one or two triples each. This equation is used for convenient curve-fitting.

$$Gauss(x) = a \exp\left(-\frac{(x-b)^2}{2c^2}\right)$$

Gaussian function [3]



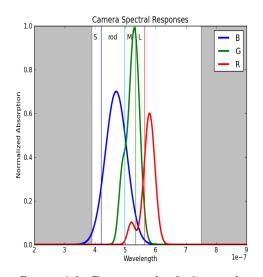


figure 15: Retinal receptor absorption

figure 16: Camera pixel absorption

The typical trichromat human has three cone photoreceptors L, M, and S. A fourth, rod photoreceptor, is labelled X in figure ¹⁵. As can be seen, all human photoreceptors absorb photons having short wavelengths. Absorption of photons at the longer end have sharp relative cutoffs such that the S cone absorbs almost no photons at wavelengths above ~550nm. The M cone cuts off at ~625nm, and L cone cuts off at ~710nm. Note the curious increase of L and M cone absorption at shorter wavelengths. All this indicates that the wavelengths in a scene are not as sharply divided into color planes as is assumed in standard image processing.

A critical function of vision is to identify readiness of a resource by its color. Regardless of the ambient

light, a ripe apple should look red. In fact, it does when viewed under a blue sky, a green forest canopy, a red sunset, or by sodium light having only two yellow and one blue spectral line. The redness of the apple does not depend on the presence of long wavelength photons. This is called color constancy and is what was described for perception under figure ¹³ and figure ¹⁴.

$$I = I_0 \left(\frac{2J_1(u)}{u}\right)^2$$

Airy equation [4]

$$u = \frac{2\pi aq}{\lambda R}$$

Airy parameter [5]

where:

 J_1 = Bessel function of the first kind

 $a = aperture\ radius$

 $q = focal\ plane\ offset$

 $\lambda = photon \ wavelength$

R = distance from aperture to focal plane

Wave superposition rules when multiple points are being projected onto an image plane. The waves from all the points are summed and the result is squared to yield the intensity map (image).

$$A = A_0 \frac{2J_1(u)}{u}$$

Airy wave equation [6]

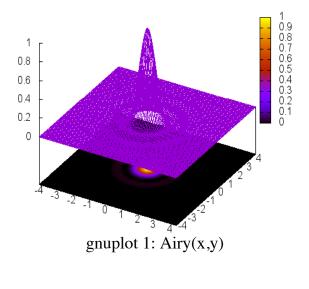
where: $A_0 = \sqrt{I_0}$

The conditions under which this occurs are special. An achromatic lens is required.

The straight lines predicted by optics between this origin identify the center of a probability distribution at the destination. The relative probability of a photon of specific energy from a specific source being absorbed within a specific tile in a grid of a tiled surface is calculated by integrating the infinitesimal probabilities over the tile.

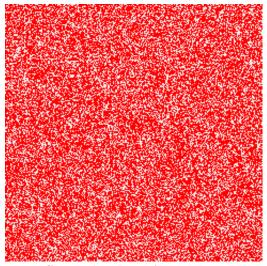
http://localhost:8001/

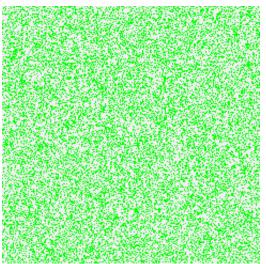
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Retinal Photoreceptor Species Mosaic





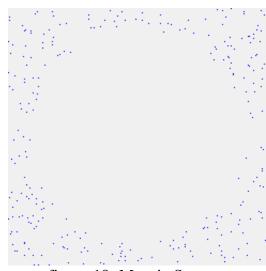


figure 17: Mosaic L cones

figure 18: Mosaic M cones

figure 19: Mosaic S cones

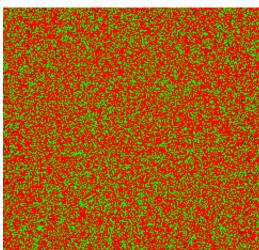


figure 20: Species Mosaic

There are four photoreceptor species in the typical trichromat human eye. Variations in species presence and distribution are found in individuals. These images are fictional characterizations of what is found in vivo. The images are produced on a rectangular grid but, in vivo, the grid is more similar to a hexagonal grid, but nowhere near reliably. These distributions are largely consistent with published data: such as the site:

http://www.cvrl.org/database/text/intros/introdens.htm

Table 1: Photoreceptor Species

Photoreceptor Species

L photoreceptors (cones shown as red) ~566nm peak absorption M photoreceptors (cones shown as green) ~533nm peak absorption I photoreceptors (rods shown as cyan) ~498nm peak absorption S photoreceptors (cones shown as blue) ~433nm peak absorption

L cones typically dominate in the macula but M cone dominance is not rare. S cones do not appear within 100μ M of center and are far fewer in number. Rods are not present in these figures and only begin to populate the retina in the outer part of the macula where they increase to 100% outside the macula. table represents the species in the typical trichromat human. Note that the distribution has no reliable pattern and is effectively random.

As is shown in figure ¹⁷ to figure ¹⁹, were the species to be treated as image planes, the effective image for each plane would have lacunae. This will be treated in a later paper focused on processing based on these effective images and the shapes of neurons. Here, it will be shown what information is present when full-spectrum scenes cause absorption events in the retina.

Here is PHP code which generates the receptor mosaic images shown here.

```
<?php
error reporting(E ALL | E STRICT);
function radius($x,$y) { return sqrt($x*$x + $y*$y); }
function species() {
    list(\$r0, \$x0, \$y0) = array fill(0, 3, 120);
             X , Y ) = array fill(0, 2, range(-$r0, +$r0));
    list(P, M, D, rs, Rmax) = [], 255, count(X), 100, radius(X), y0)];
   $image = ['L' => '' , 'M' => '' , 'S' => '' , 'LMS' => '' ];
    count = ['L' => 650], 'M' => 340], 'S' => 10], 'I'
                                                                  => 0 1;
    somes = ['L' => [sm,0,0], 'm' => [0,sm,0], 's' => [0,0,sm]
                                                                        ];
    foreach (array keys($image) as $k)
       ${'im'.$k} = $image[$k] = @imagecreatetruecolor($D, $D)
       or die("{$k} mosaic fail");
    foreach ($image as $im)
       imagefill($im, 0, 0, imagecolorallocate($im, 240, 240, 240));
    foreach ($cones as $cone => $channel) {
       list($r, $q, $b)
                          = $channel:
       $$cone
                          = imagecolorallocate($imLMS, $r, $q, $b);
       ${$cone.'L'}
${$cone.'M'}
                          = imagecolorallocate($imL , $r, $q, $b);
                          = imagecolorallocate($imM , $r, $q, $b);
                          = imagecolorallocate($imS , $r, $g, $b);
       ${$cone.'S'}
       if (($N=$count[$cone])) $P = array merge($P, array fill(0, $N, $cone));
    foreach ($X as $x1) {
       $x = $x1+$x0;
       foreach ($Y as $y1) {
           y = y_1 + y_0;
           r = radius(x1, y1);
           $LMS = ($LM = $count['L'] + $count['M']) + $count['S'];
           c = P[rand(0, ((r < rs) ? LM : LMS) - 1)];
           imagesetpixel($image[$c], $x, $y, $$c); // Species mosaic
       }
    foreach ($image as $key => $im) imagepng(
                                              $im, "species{$key}.png");
    foreach ($image as
                             $im) imagedestroy($im
                                                                    );
species();
Listing 1: Generating the mosaic
```

Spectral Encoding Constraints

Retinal photoreceptors respond to photons across the entire visual spectrum. To determine what a retinal response is to a scene lit by sunlight it is necessary to compute the dot product of the spectrum presented to a photoreceptor with its absorption spectrum. The point of this paper is to compute that dot product and show the effect this has on each of the individual cone mosaics and on the combined mosaics.

For the vast majority of spectra, it is sufficient to specify a source as either a set of blackbodies or as a set of gaussians. Usually a single blackbody is sufficiently specified as an amplitude and a temperature (two parameters). Usually a single gaussian is sufficiently specified as an amplitude, a peak λ , and a width (three parameters).

Synthetic images are produced by summing wave equations and squaring the result, so it is convenient to use the square root of peak intensity as the amplitude. An image can be fully specified with spectral precision from pixels composed from their spectral components.

Pixels locations may be either specified on pixel groups randomly scattered over the image, or as raster images where the location is implied by its position in the raster line set.

The former permits a full lower-quality image to be delivered early with improving fidelity as more pixels arrive. The latter requires full delivery of all pixels before the full image may be seen. In the former case, a spectral specification is given followed by a sequence of (x,y) pixel coordinates. A 4096x4096 pixel image can use 12 bits per dimension or 3 bytes per pixel. First priority of presentation should be given to generating a neutral background. Second priority should be given to larger differences across boundaries. Last priority should be given to field filling operations.

Digital cameras are unable to produce images of this type since they are restricted to sampling 3 narrow spectral bands. Older photographs are also unable to produce these images for similar reasons. The only feasible manner of production of test images suitable for analysis of vision is synthesis.

As will be shown, acceptable synthetic images can be produced and their effects on retinal photreceptors properly modelled.

2 Methods

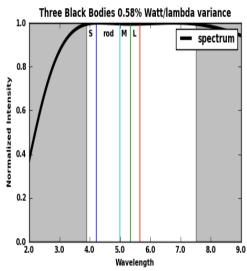
Full spectrum image file representation.

Currently, there is no popular stored image format capable of storing a full spectrum image of the sort needed for this analysis. It is possible to specify a format for use in this paper. The format for a given pixel may be given as a list of specifications. Each specification has 1 bit to identify the coefficients as either blackbody figure ¹³ equation or gaussian equation (a variation on equation). If identified as

blackbody, a pair of (I_0,T) coefficients or (a,b) follows. If identified as gaussian, an $(I_0, \lambda_{peak}, RMSwidth)$ or (a,b,c) coefficient triple follows.

$$I(\lambda) = I_0 \exp\left(-\frac{(\lambda - \lambda_{peak})^2}{2RMSwidth^2}\right)$$
 Gaussian function in λ [7]

The spectrum of a pixel may be fully described as a list of components: (B:((a1,b1),(a2,b2)...), G:((a3,b3,c3),(a4,b4,c4)...)). Each coefficient is a floating point number limited to a small range. Using the "half" float (16 bits), it is possible for blackbody specifications to occupy 32 bits and gaussian to occupy 48 bits. I_0 Cannot be negative, so the sign bit of coefficient a may be used to indicate whether it is a G (gaussian) or B (blackbody). For shorthand, uppercase letters will indicate Blackbody coefficients when the first coefficient is negative. Here is a fanciful pixel spectrum: (A1,B1,a2,b2,c2,a3,b3,c3,A4,B4). In most cases, only one or two components will be used. In no case shown in this paper will blackbody and gaussian components be mixed.



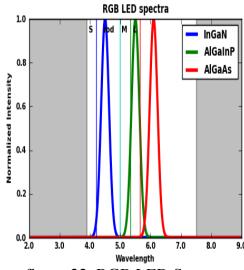


figure 21: White Body Spectrum

figure 22: RGB LED Spectrum

An example is the white body spectrum figure²¹ where intensity variation over the entire visible spectrum is less than 1%. This is expressable as the 96 bit or 12 byte (A1,B1,A2,B2,A3,B3) with values (-1e-2,8.7e+3,-3.226e-2,5.6e+3,-1.732e+0,3e+3). Note the negative values for A1, A2, and A3 indicating black body coefficients.

Another example is the spectral composition of a white LED pixel when using LEDs of types R:AlGaAs, G:AlGaInP, B:InGaN. The b coefficient is given in nanometers. figure²². In this figure, each component is given by a single gaussian.

 $(I_R,610,0.18e-7,I_G,550,0.18e-7,I_B,450,1.7e-7,0.18e-7)$

Typically, images are laid out as either raster sequences of pixels or as vector graphics. Another alternative, used here, is to give the coordinates of a pixel at which a spectrum is expressed. With (x,y) expressed as 12 bits for each coordinate (24 bits) a pixel is expressed as (x,y,a1,b1,c1,a2,b2,c2...). 3 bytes for coordinates and 6 bytes for each gaussian or 4 bytes for each blackbody component. This pixel spectrum may be used for spectral calculations such as multiplying the probabilities of capture by a photoreceptor by the probabilities of photons arriving from a scene. An S photoreceptor figure 15 takes 9 bytes. An M and L photoreceptor each take 15 bytes for complete spectral representation. For instance with positive a1, and a2 for gaussian coefficients:

```
List 1: Spectra for human cones

• L cone spectrum (x1,y1,I0,564,0.58e-7,0.25*I_0,400,0.58e-7)

• M cone spectrum (x2,y2,I0,534,0.58e-7,0.25*I_0,400,0.58e-7)

• I rods spectrum (x3,y3,I0,498,0.58e-7,0.25*I_0,400,0.58e-7)

• S cone spectrum (x4,y4,I0,420,0.58e-7)
```

The spectra of figure ¹⁵ were generated using these coefficients and they may be compared favorably with published absorption spectra for human photoreceptors, notably Bowmaker J.K. and Dartnall H.J.A.².

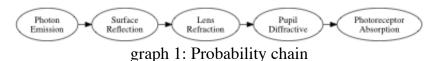
While the stored form of a full photograph would be expanded by about a factor of 4 with use of this representation, an image composed of photons from point sources may actually be far smaller than with traditional RGB digital images yet capable of expressing the full spectra required for analyzing vision in natural light settings.

Photon probability chain

Probabilities for photon capture are products of probabilities for every step between emission and absorption. The spectrum of blackbody emission E_{λ} is a probability function of wavelength. Objects have a surface reflectance spectrum S_{λ} . The cornea and lens have a refraction spectrum L_{λ} at each retinal photoreceptor. The pupil has a diffraction spectrum P_{λ} at each retinal photoreceptor where it is absorbed. Finally, each species of photoreceptor has an absorption spectrum A_{λ} . The relative probability of a photon from the point source being absorbed by the particular photoreceptor is shown in equation⁸.

$$E_{\lambda} * S_{\lambda} * L_{\lambda} * P_{\lambda} * A_{\lambda}$$

Probability chain [8]



In effect, each spectrum between emission and absorption modifies the image as absorbed. No single step in the chain stands alone as dominating the result. Isotropic emission from a blackbody doesn't alter the course of a photon to the photoreceptor. Isotropic reflection, also, doesn't differentially

change photon pathways. Refraction performs an Affine transform with the pattern seen for short wavelength photons displaced further to the outside. Diffraction performs two function: convolution with a spatially limited discrete Airy kernel followed by an affine transform with long wavelength photons displaced further to the outside.

The resulting function of wavelength forms a probability pattern which may be converted to a wave equation for superposition. Since the final step in the chain is multiplication by the absorption spectrum of the photoreceptor, the apparent image incident on each species of receptor differs substantially from that for other species.

RGB test pattern

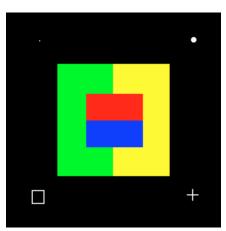


figure 23: RGB test pattern

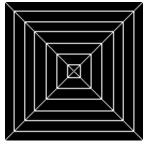


figure 24: Another RGB pattern



figure 25: As incident on retina

3 Results

4 Discussion

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\$id: a keyword to use when referencing this equation;

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equation defaults ...

No defaults ...

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5 Acknowledgments

6 Literature

- 1. The Colors Of Things, Jerome Y. Lettvin et al, Lettvin et al, Scientific American, 1986, September, 255.3, 84-92
- 2. Visual pigments of rods and cones in a human retina, Bowmaker J.K. and Dartnall H.J.A., J. Physiol., 1980, 298, 501-511

7 Appendices

8 Missing