# Understanding Neural Networks for Image Segmentation

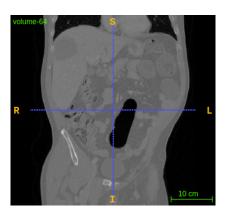
#### Jonas Actor

Rice University

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## Target application: medical image segmentation



Abdominal CT scan



Liver and tumor segmentation

#### Why automate?

- · needed for treatment plans
- · costly (time+effort) to perform by hand
- less interobserver variability → better accuracy

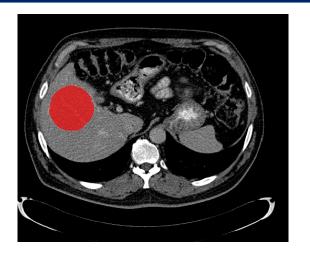
errors in segmentation = errors in radiation treatment

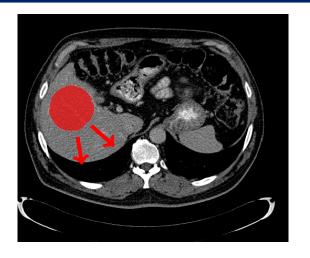
#### Goal: understand why CNNs work so well

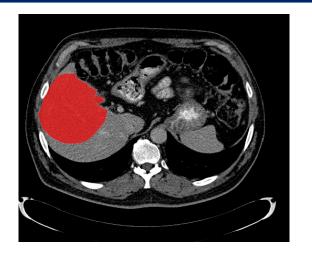
- Compare PDEs to CNNs
- Build CNNs like PDEs
- Analyze kernels and explain performance
  - Entrywise comparison
  - SVD comparison

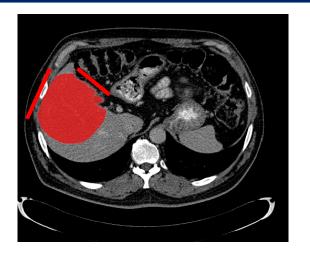
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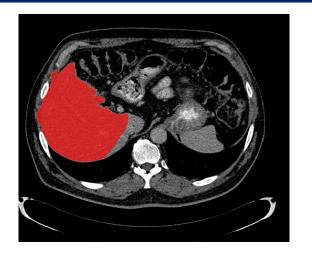
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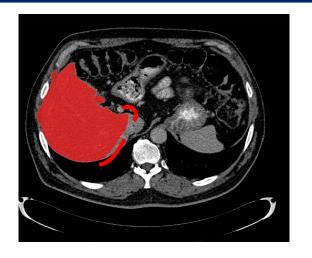














#### Classical Approach: Level Set Equation

$$\partial_t u - \alpha \underbrace{g_l}_{\text{balloon force}} - \beta \underbrace{g_l \kappa(u)}_{\text{mean curvature}} - \gamma \underbrace{\nabla g_l \cdot \nabla u}_{\text{convection}} = 0$$

- Well-established theory to analyze approximation, stability
- Upwind finite differences + fast marching method
- · Semiautomated: requires initialization by user
- Works for simple problems only: relies on edge information

# Comparison: LSE vs CNN

	Can analyze?	Accurate?
LSE	yes	sometimes
CNN	no	yes

Goal: accurate method we can analyze

#### Similarities between LSE and CNN

	LSE	CNN		
Convolution	finite difference kernel	learned kernel		
	$\frac{1}{h^2} \begin{bmatrix} 0 & 1 & 0 \\ 1 & -4 & 1 \\ 0 & 1 & 0 \end{bmatrix}$	$\begin{bmatrix} k_{11} & k_{12} & k_{13} \\ k_{21} & k_{22} & k_{23} \\ k_{31} & k_{32} & k_{33} \end{bmatrix}$		
ReLU	upwind scheme	activation function		
	$\max(0, D^+ * u) + \min(0, D^- * u)$	$\max(0,K*x+b)$		

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#### Build a CNN like a LSE solver

#### Level Set Equation → Level Set Network

- Discretize Level Set Equation
  - Explicit forward Euler in time
  - Upwind finite differences in space
- ② Forward Euler → residual skip connections
- ③ Upwind finite differences → convolutions and ReLU

#### Forward Euler time discretization

$$\frac{u^{(t+1)} - u^{(t)}}{\delta_t} - \alpha g_I - \beta g_I \kappa(u^{(t)}) - \gamma \nabla g_I \cdot \nabla u^{(t)} = 0$$

#### Edge indicator $g_l$

$$g_I(x) = \frac{1}{1 + \|\nabla I(x)\|^2}$$

becomes

$$g_I(x) = \frac{1}{1 + \sum_{j=1}^{N_{conv}} (\sigma_j * I(x))^2}$$

#### Convection term: Upwind Finite Differences

$$\begin{split} \nabla g_{I} \cdot \nabla u^{(k)} &= \max\{0, \partial_{x} g_{\mathcal{I}}\} D_{x}^{+} * u^{(k)} - \max\{0, -\partial_{x} g_{\mathcal{I}}\} D_{x}^{-} * u^{(k)} \\ &+ \max\{0, \partial_{y} g_{\mathcal{I}}\} D_{y}^{+} * u^{(k)} - \max\{0, -\partial_{y} g_{\mathcal{I}}\} D_{y}^{-} * u^{(k)} \\ &= \text{ReLU}(\partial_{x} g_{\mathcal{I}}) D_{x}^{+} * u^{(k)} - \text{ReLU}(-\partial_{x} g_{\mathcal{I}}) D_{x}^{-} * u^{(k)} \\ &+ \text{ReLU}(\partial_{y} g_{\mathcal{I}}) D_{y}^{+} * u^{(k)} - \text{ReLU}(-\partial_{y} g_{\mathcal{I}}) D_{y}^{-} * u^{(k)} \end{split}$$

## Curvature term $\kappa(u)$

$$\kappa(u^{(k)}) = \nabla \cdot \left( \frac{\nabla u^{(k)}}{\|\nabla u^{(k)}\|} \right)$$

becomes

$$egin{aligned} 
abla \hat{u}^{(k)} &= \sum_{i=1}^{N_{conv}} 
ho_i * u^{(k)} \ \kappa(u^{(k)}) &= \sum_{j=1}^{N_{conv}} \sigma_j * rac{
abla \hat{u}^{(k)}}{\|
abla \hat{u}^{(k)}\| + arepsilon} \end{aligned}$$

#### Implementation

- If convolution kernels are finite difference kernels, we recover LSE
- If convolution kenrels are learned, we construct LSN
- Python + Tensorflow / Keras implementation
- Out LSE agrees with ITK-SNAP, a common LSE-segmentation program

#### LSN: Results

K-Fold	LSE	LSN Test	LSN Validation	UNet
0	0.736	0.837	0.619	0.912
1	0.600	0.847	0.729	0.919
2	0.483	0.116	0.005	0.874
3	0.730	0.827	0.606	0.895
4	0.643	0.831	0.596	0.915
Avg	0.604	0.692	0.511	0.903
Avg $-\{2\}$	0.640	0.837	0.638	0.911

Table: DSC scores for each fold, from training the level set network.

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#### Identification of Kernels

- Are CNN convolution kernels finite difference stencils?
- Are they close to finite difference stencils?
- What about other standard image processing kernels?

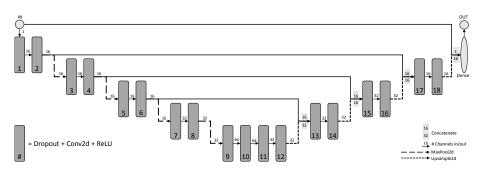
#### Numerical analysis kernels

- Laplacian
- Edge detection
- Identity

#### Image processing kernels

- Gaussian blur
- Local mean
- Sharpen

#### Setup of CNN



Trained on MICCAI LiTS 2017 dataset for liver segmentation

## Kernel Analysis: Comparing entries

- For each layer, separate each channel's  $3 \times 3$  convolution kernel
- Flatten each 3  $\times$  3 kernel into a vector  $\in \mathbb{R}^9$
- Cluster with k-means
- Project down using PCA
- Project known numerical analysis and image processing kernels

## Kernel Clustering Results

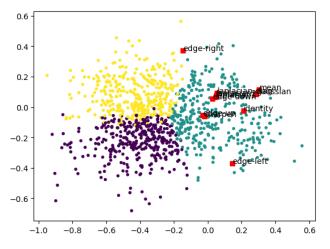


Figure: Convolution Layer 11 (encoder)

## Kernel Clustering Results

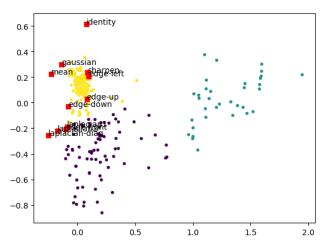


Figure: Convolution Layer 14 (decoder)

- **1** Construct matrix  $A_{[K]} \in \mathbb{R}^{n_x n_y \times n_x n_y}$  describing convolution with K
- 2 Compute singular values of linear operator
- 3 Compute singular values of clinical image processing kernels
- Assign closest clinical feature F that has smallest spectral distance to K

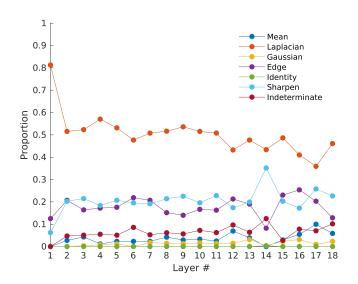
Kernel 
$$K = \begin{bmatrix} k_{-1,-1} & k_{-1,0} & k_{-1,1} \\ k_{0,-1} & k_{0,0} & k_{0,1} \\ k_{1,-1} & k_{1,0} & k_{1,1} \end{bmatrix}$$

For 
$$i \in \{-1, 0, 1\}$$
,

$$\begin{split} A_{[K]} &= U_K \Sigma_K V_K^T & \forall K \in \{ \text{layers} \} \\ A_{[F]} &= U_F \Sigma_F V_F^T & \forall F \in \{ \text{features} \} \end{split}$$
 find  $\underset{F \in \{ \text{features} \}}{\text{arg min}} \| \Sigma_K - \Sigma_F \|_1$ 

Label as 'indeterminate' if not within 10% of largest singular value

#### Kernel Analysis Results



#### Conclusions

- Level Set Equation ≠ Level Set Network ≠ UNet
- Framework for using same operations (convolutions + ReLU) for both NNs and PDEs
- Framework for GPU-supported finite differences in Tensorflow
- Examine how learned CNN kernels change across different layers

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