

# FAST SOLUTIONS TO THE BLOCH-TORREY PARTIAL DIFFERENTIAL EQUATION



Simulation of Cerebral Magnetization

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# THE BLOCH-TORREY EQUATION

- The Bloch-Torrey equation is a fundamental equation in MRI physics which describes how the *complex* transverse magnetization changes through time



$$\frac{dM}{dt} = D \cdot \nabla^2 M - (R_2 + i\delta\omega) \cdot M$$

- Where

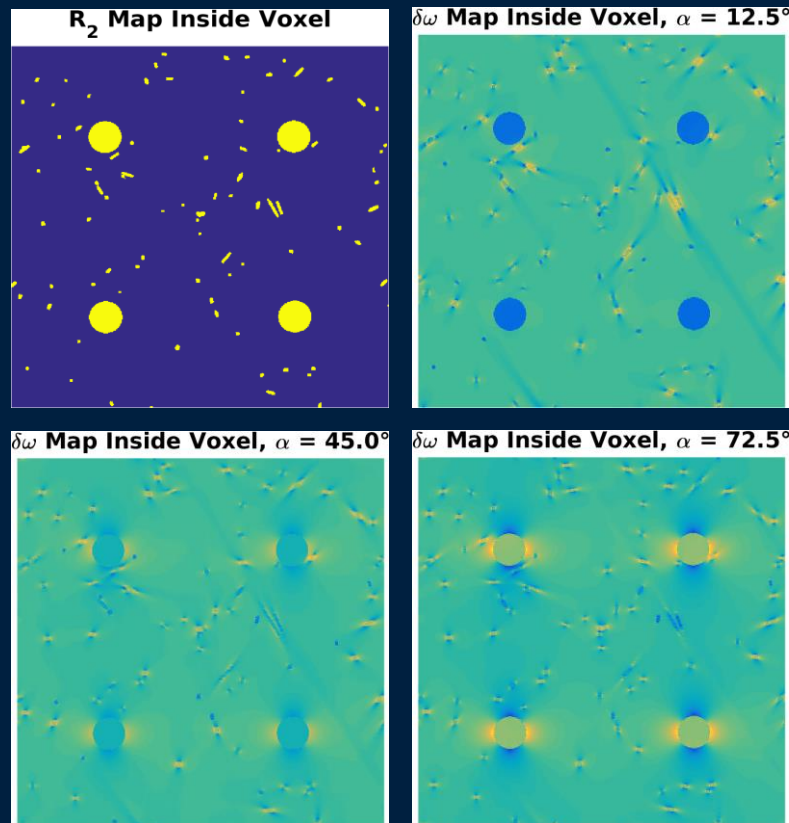
$$M := M_x + iM_y$$

- Therefore, this problem must be solved in complex variables

# GEOMETRY

$$\frac{dM}{dt} = D \cdot \nabla^2 M - (R_2 + i\delta\omega) \cdot M$$

- Equation is solved in a finely discretized 3D box, called a “voxel”
- $R_2$  is piecewise constant, and  $\delta\omega$  is piecewise smooth
  - Problem is very discontinuous!



# FAST SOLUTIONS

$$\frac{dM}{dt} = D \cdot \nabla^2 M - (R_2 + i\delta\omega) \cdot M$$



- In addition to solving the equation, the resulting signal (integral of  $M$ ) must be fit to observed data
- Involves thousands of system solves

# FAST SOLUTIONS

$$\frac{dM}{dt} = D \cdot \nabla^2 M - (R_2 + i\delta\omega) \cdot M$$



- Currently, the best trade off of accuracy vs. speed is to use (relatively crude) “splitting methods”
- Essentially, based on the approximation

$$e^{(A+B)t} \approx e^{\frac{At}{2}} e^{Bt} e^{\frac{At}{2}}$$

- For linear operators  $A$  and  $B$ 
  - We take  $A = -(R_2 + i\delta\omega)$  and  $B = D\nabla^2$ , and use the fact that the action of the exponential of  $D\nabla^2 t$  (i.e. the solution of the heat equation) is the convolution with a Gaussian kernel, and can be performed efficiently via the FFT