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# Computational Neuroscience

# How many neurons can we see with current spike sorting algorithms?

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#### HIGHLIGHTS

- ► Spike sorting algorithms are limited in the number of single units they can detect.
- ▶ The maximum number of correctly identified neurons stands between 8 and 10.
- ► Sparse neurons are strongly affected by this limitation.
- ► Further development of algorithms is needed to address sparse neurons detection.

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#### ABSTRACT

Recent studies highlighted the disagreement between the typical number of neurons observed with extracellular recordings and the ones to be expected based on anatomical and physiological considerations. This disagreement has been mainly attributed to the presence of sparsely firing neurons. However, it is also possible that this is due to limitations of the spike sorting algorithms used to process the data. To address this issue, we used realistic simulations of extracellular recordings and found a relatively poor spike sorting performance for simulations containing a large number of neurons. In fact, the number of correctly identified neurons for single-channel recordings showed an asymptotic behavior saturating at about 8–10 units, when up to 20 units were present in the data. This performance was significantly poorer for neurons with low firing rates, as these units were twice more likely to be missed than the ones with high firing rates in simulations containing many neurons. These results uncover one of the main reasons for the relatively low number of neurons found in extracellular recording and also stress the importance of further developments of spike sorting algorithms.

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# 1. Introduction

Complex brain processes are encoded by the activity of relatively large neural networks and, consequently, the study of these processes can benefit from the simultaneous recording and analysis of the firing patterns from large populations of neurons (Douglas and Martin, 1991; Brown et al., 2004; Harris et al., 2003; Buzsaki, 2004; Quian Quiroga and Panzeri, 2009). In addition, applications using Brain Machine Interfaces and neural prostheses could significantly profit from the possibility of recording large numbers of neurons, as this allows the decoding of more complex and precise motor actions (Donoghue, 2002; Carmena et al., 2003; Chapin, 2004; Musallam et al., 2004; Velliste et al., 2008; Nicolelis and Lebedev, 2009). The development of multiple electrode recording probes (Maynard et al., 1997; Blanche et al., 2005; Keefer et al., 2008) and spike sorting algorithms (Letelier and Weber, 2000; Pouzat et al., 2002; Quian Quiroga et al., 2004; Zhang et al., 2004; Rutishauser et al., 2006;

Vargas-Irwin and Donoghue, 2007) have provided an increasing number of identified neurons from multiple-site recordings, reaching values of dozens or even hundreds of simultaneously recorded neurons over long periods of time (Carmena et al., 2003; Buzsaki, 2004; Blanche et al., 2005; Jackson and Fetz, 2007; Tolias et al., 2007). In the case of single channel recordings, improvements of spike sorting algorithms have allowed identifying up to half a dozen neurons, as it is the case with data from the human medial temporal lobe (Quian Quiroga et al., 2005, 2007).

In spite of these advances, based on the effective radius seen by an electrode and the density of neurons, it has been estimated that the number of identified neurons per channel should be one or two orders of magnitude higher (Henze et al., 2000; Buzsaki, 2004). Different factors have been proposed to account for the relatively low number of identified neurons. In particular, it was suggested that this could be due to tissue damage caused by the insertion of the electrodes in the recording area (Claverol-Tinture and Nadasdy, 2004), or the electrical insulation caused by the substrate of the probe (Moffitt and McIntyre, 2005). Another possible reason for this mismatch is the presence of sparsely firing neurons, which are unlikely to be detected because they are silent most of the time

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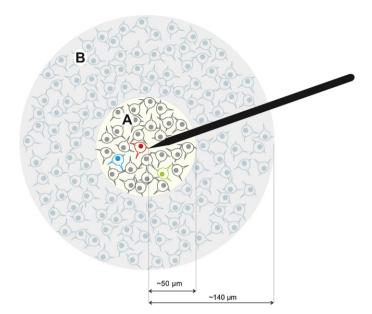
(Buzsaki, 2004; Shoham et al., 2006). Nonetheless, even the combination of these effects can hardly account for the large gap between the expected number of units and the ones obtained in real data. In this study we evaluate yet another possibility, namely, that the relatively low number of detected neurons could be due to limitations of the spike sorting algorithms.

Let us illustrate this issue with a simple calculation. Approximating the neuron by a dipole source, following Coulomb's law the amplitude decays as  $v \sim 1/r^2$ , as a function of the distance. We can also consider that spikes of about 60  $\mu$ V are produced by neurons at a distance of about 50 µm - the maximum distance (and minimum amplitude) at which single units are identified (Buzsaki, 2004). Taking a density of 300,000 neurons/mm<sup>3</sup> (as in the rat hippocampus; Henze et al., 2000), it immediately follows that there should be more than 30 neurons firing spikes with an amplitude between 60 and 70 µV, at the threshold of single unit detection, and about 10 neurons firing (relatively large) spikes, within 100 and 110 µV. So, within a small amplitude range of 10 µV there are several neurons whose spikes could hardly be separated by their amplitudes (i.e. using a spike sorter based on amplitude discrimination) given the background noise. It is also likely that more sophisticated spike sorters that extract features of the spike shapes (beyond their amplitude) will also miss at least some of these neurons, as we report below.

With some notable exceptions (see Harris et al., 2000 and Wehr et al., 1999 for examples of simultaneous extra- and intra-cellular recordings), a major limitation in the evaluation of spike sorting algorithms with real data is that there is no 'ground truth' to univocally obtain a measure of an algorithm's performance. Consequently, the quantification of spike sorting results requires the use of synthetic datasets, which also offer the possibility of controlling parameters such as the signal to noise ratio, the firing rate of the units and the characteristics of the different spike shapes, thus allowing a reliable measure of the algorithm performance under different recording conditions. In line, synthetic datasets were used in several previous works (Letelier and Weber, 2000; Quian Quiroga et al., 2004; Zhang et al., 2004; Vargas-Irwin and Donoghue, 2007). However, these spike sorting outcomes were tested with simulations containing only a few single-units. Therefore, it remains unknown how these algorithms would perform on datasets with larger number of neurons, as it can be expected from the considerations discussed above. To address this issue, in this study we systematically evaluated the spike sorting performance using simulations of extracellular recordings with increasing number of neurons, also focusing on the detection of sparsely firing neurons.

# 2. Materials and methods

Neurons contributing to the extracellular recording can be seen as generators of electric signals that are captured by the electrode placed in the brain tissue. When activated, each of these generators produce action potentials (or spikes) with a particular amplitude and shape (Gold et al., 2006). A simplified scheme of the recording with an electrode implanted in neural tissue is shown in Fig. 1. In the area surrounding the tip of the electrode (region A, with white background) the magnitude of the spikes is considerably higher than the background noise and it is therefore possible to detect and identify the firing of the neurons with high accuracy. The neurons in red, green and cyan represent active neurons in this area - up to 50 µm from the electrode tip (Buzsaki, 2004) - recorded by the electrode and sorted according to their shapes. The remaining neurons in this area (in gray) represent neurons whose activity is not detected due to their very low firing rate (see Shoham et al., 2006). The area in light gray (region B) contains neurons close enough to the tip of the electrode to produce spikes larger than the overall



**Fig. 1.** Extracellular recordings. Spikes in the area close to the electrode tip (region A) are considerably higher than the background noise, and are therefore easily detected and sorted. The neurons in red, green and cyan represent 3 active neurons recorded by the electrode and sorted by the algorithm. The neurons in gray represent those that fire very sparsely and are not detected. Neurons in the light gray area (B) produce spikes that are larger than the background activity, but not large enough to be individually sorted. The spikes fired by these neurons are usually grouped together in a multiunit cluster. Neurons outside this area contribute to the background noise.

noise level, but too small to be individually sorted. The spikes fired by these neurons are usually grouped together and are considered to be a 'multiunit cluster'. Neurons further away from the electrode tip – outside area B, i.e. more than 140  $\mu m$  from the electrode tip (Buzsaki, 2004) – produce spikes that are too small to be detected and they only contribute to the background noise.

To evaluate the spike sorting performance with different numbers of neurons, we created a total of 95 simulations of 10 min of extracellular recordings. Each of these simulations contained background noise, multiunit activity and between 2 and 20 neurons (5 simulations for each case). Following previous studies from our group (Quian Quiroga et al., 2004; Martinez et al., 2009), the noise, multiunit and single unit activities were generated using a database of 594 different average spikes compiled from recordings of monkey basal ganglia and neocortex, as detailed below. In the simulated data, the spike times and labels of the multiunit and the single unit spikes were stored for subsequent analyses.

The data was first generated with a sample rate of 96,000 Hz and it was then decimated by a factor of 4, thus giving a sampling rate of 24,000 Hz. This replicated the fact that in real recording conditions spikes occur at continuous time points, thus introducing misalignments and making spike sorting more challenging.

# 2.1. Simulation of the background noise

For each simulation, the first step was to generate the background noise by modeling the overall contribution of distant neurons (neurons at a distance larger than 140 µm from the electrode tip; area outside the circle shown in Fig. 1). To do this, we superimposed at random times a large number of spikes selected randomly from the average spike shapes in the database. As in previous works (Quian Quiroga et al., 2004; Martinez et al., 2009), the total number of spikes used to build the noise was half the number of samples during the generation of the signal, prior to the downsampling process, *i.e.* each second of simulation was generated by the superimposition of 48,000 spikes. The amplitude of each of

these spikes was scaled by a value randomly selected from a normal distribution ( $\mu$  = 1,  $\sigma$  = 0.2). After superposition of all the spikes, the mean of the resulting signal was then subtracted and scaled to a standard deviation of 0.1.

#### 2.2. Simulation of multiunit activity

The simulated signals also included multiunit activity, generated by the spikes fired by neurons in region B of Fig. 1. Although the aim of our study was to analyze the clustering performance for the single units, the multiunit activity was introduced in order to replicate a more realistic scenario where the presence of large multiunit clusters increased the complexity of the sorting process.

To simulate the multiunit activity we added the contribution of 20 different spike shapes randomly selected from the database to the background noise. The amplitude of the spikes used to construct the multiunit activity was fixed to 0.5, a value close to the detection threshold (see below). As typically found in the experimental data, the firing rate of the multiunit was set to 5 Hz, *i.e.*, each of the 20 neurons generating the multiunit followed an independent Poisson distribution with a mean firing rate of 0.25 Hz.

# 2.3. Simulation of single unit activity

Single unit activity is given by the firing of neurons close-by the electrode tip (region A in Fig. 1). The time of firing of the single units was modeled following a Poisson distribution with a mean firing rate randomly selected between 0.1 and 2 Hz (uniform probability). The amplitude of each unit was randomly selected from a normal distribution ( $\mu$  = 1.1,  $\sigma$  = 0.5), capped to values within the range 0.9–2 to resemble the amplitude distribution (referred to the noise level) found in real data (Quian Quiroga et al., 2007). For the sake of clarity we did not to include overlapping spikes in our simulations (*i.e.* spikes had to be more than 3 ms apart from each other). It is likely that the limitation of spike sorting algorithms described in our results will be even larger when considering overlapping spikes.

#### 2.4. Performance evaluation

Three expert operators performed an independent (and blind) spike sorting of the 95 simulations - each with 2-20 neurons using Wave\_clus (Quian Quiroga et al., 2004). This software offers a combination of properties specially suited for our study: (i) the detection threshold is based on the median of the absolute value of the signal, thus offering a robust estimation of the background noise and reducing the dependence on the amount (and amplitude) of the spikes present in the signal; (ii) the number of clusters obtained is determined automatically; (iii) the algorithm does not make a priori assumptions about the shape of the clusters; and (iv) it is able to identify clusters with very different sizes, which is wellsuited for clustering sparsely firing neurons. The sorting process for each simulation was performed automatically using the default parameters of Wave\_clus (Quian Quiroga et al., 2004). When the automatic clustering was not satisfactory, the operators optimized the results using the Wave\_clus GUI (by changing the clustering temperature, merging or rejecting clusters).

For each spike sorting outcome, we quantified the number of correctly and incorrectly identified neurons using the following criteria. *Hits* referred to correctly identified clusters fulfilling two conditions: (1) at least 50% of the spikes corresponded to the same neuron; and (2) the number of detected spikes were, at least, 50% of the number of generated spikes for this particular neuron. As shown in Fig. S1, other choices gave similar results. The number of *misses* was quantified as the total number of generated neurons

minus the number of hits. In addition, the clusters identified by the user that did not fulfill condition (1) or (2) were considered to be *false positives*, and they corresponded to spurious subdivisions of the units present in the simulation.

Given the previously reported problems in separating clusters with relatively large size differences (Ott et al., 2005), we also divided our units into low-firing and high-firing neurons for additional analysis. We defined low-firing neurons as those with a firing rate below 0.5 Hz (less than 300 spikes in the 10 min of simulated data) and high-firing neurons as the rest, and evaluated the performance for both populations separately. Due to the random mean firing rate assigned to each unit, for each on of the simulations with a certain number of units we obtained different number of low-firing and high-firing neurons. Therefore, to compare both populations we defined the performance ratio as the number of hits with high- (low-) firing neurons, divided by the total number of high- (low-) firing neurons present in the simulation. Ratios for misses and false positives were defined in a similar way.

# 2.5. Statistical analysis

The spike sorting performance for the low- and high-firing neurons was compared using a two-way ANOVA (Test 1). The two independent variables were the number of neurons in each simulation (from 2 to 20) and the neuron type (*i.e.* low-firing or high-firing). The repeated measures were the corresponding performance ratios (hits, misses or false positives).

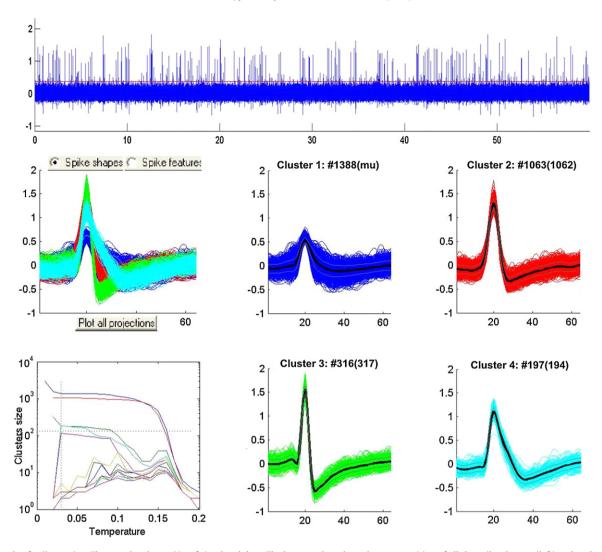
To ensure that there was no statistical difference between results obtained by the three experts we tested for inter-rater reliability using a Fleiss' kappa coefficient for hits-false positives results as well as for the hits for the low-firing and high-firing units (Test 2).

#### 3. Results

#### 3.1. Single case examples

An example of the simulated data and the spike sorting performed by one of the experts is shown in Fig. 2. The top plot shows 60 s of raw signal and the bottom plots show the (correctly) sorted units: 3 single units (clusters 2, 3 and 4) and 1 multiunit (cluster 1). The simulation contained background noise, a multiunit activity cluster 2916 spikes, and 3 single units (classes 1, 2 and 3) with amplitudes 1.38, 1.69 and 1.22 and firing rates 1.91, 0.52 and 0.35 Hz, which gave 1063, 317 and 194 spikes, respectively. For the multiunit, only 1338 out of 2916 spikes were correctly identified by the user. The multiunit cluster contained 50 false detections and the remaining 1522 spikes did not cross the detection threshold. The detection and sorting performance of single units was, as expected, much more accurate than the one of multiunit. For cluster 2 the operator detected 1062 of the 1063 spikes generated for this unit plus a single spike from another unit. For cluster 3 the operator detected 316 of the 317 generated spikes. For cluster 4 the operator detected all the 194 spikes, plus 3 extra spikes from

Fig. 3 shows a more complex simulation with 1 multiunit and 6 single units. In this case, the simulation was originally generated with a multiunit containing a total of 2870 spikes and the single units (classes 1–6) had amplitudes 1.95, 1.35, 1.19, 1.08, 1.57 and 1.3, and firing rates 0.24, 0.85, 1.54, 1.02, 0.43 and 1.19 Hz, respectively. The operator clustered a multiunit (cluster 2) and 4 single units (clusters 1, 3, 4 and 5). For clusters 3 and 4 the operator correctly identified 676 and 508 spikes, respectively. For cluster 5 the operator detected all the 134 spikes and



**Fig. 2.** Example of spike sorting. The top plot shows 60 s of simulated data. The bottom plots show the superposition of all the spike clusters (left) and each of the sorted clusters, corresponding to one multiunit (cluster 1) and 3 single units (clusters 2, 3 and 4). The number on top of each plot indicates the number of spikes generated (in brackets) and detected by the user.

2 more spikes from another neuron. In contrast, cluster 1 was incorrectly identified as a single unit. In fact, this cluster contained the activity of 3 different neurons (shown in the inset of the figure) with quite overlapping shapes that appeared as a single cluster to the operator. This error was partially due to the presence of other neurons in the simulation. The clustering of only these 3 spike shapes indeed gave the correct result (see Fig. S2).

# 3.2. User's performance

Three different operators blindly sorted the 95 simulations generated for this study (see Section 2). Table 1 shows the number of hits for all simulations, for each operator separately. Despite some individual differences, all users had a similar overall performance, significantly different from coincidental agreement (Test 2 for hits minus false positives, kappa=0.33, z=16.67,  $p<10^{-5}$ ), reaching a similar asymptotic average number of hits in their sorting results. This suggests that the results obtained for the different number of neurons were related to the inherent characteristics of the spike sorting process and were not significantly influenced by the subjectivity and potential biases

of each operator. Similar results were found when dividing the results by firing rates, with significant coincidences for both high-firing and low-firing units (Test 2, high-firing hits: kappa = 0.55, z=25.87, p<10<sup>-5</sup> low-firing hits: kappa = 0.56, z=15.09, p<10<sup>-5</sup>). Table 2 presents the number of false positives. Altogether, the number of false positives was relatively low, thus indicating that overclustering (*i.e.* splitting the activity of a single source – simulated neuron – into 2 or more clusters) was

# 3.3. Number of identified neurons

Fig. 4a shows the average number of hits as a function of the number of generated neurons. For simulations with a few neurons the number of detected clusters was nearly perfect (the ideal performance marked by the dashed line). For simulations with more neurons the performance decayed compared to the ideal performance, reaching an asymptotic value at about 8–10 correctly identified neurons. Fig. 4b displays the number of misses and false positives for the different number of generated neurons. The curve with the misses shows a complementary behavior to the one of the number of hits. It is negligible for low number of units and it rises as

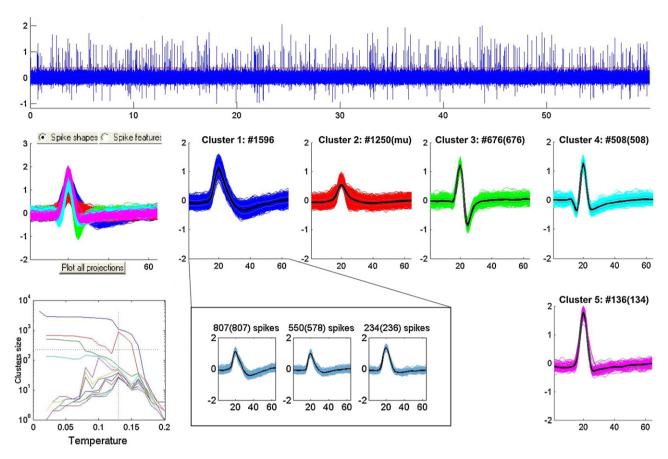


Fig. 3. Spike sorting with a large number of units. For this simulation, the operator incorrectly identified one multiunit (cluster 2) and 4 single units (clusters 1, 3, 4 and 5). However, cluster 1 was formed by 3 different neurons (inset).

the number of generated neurons increase. In fact, the dotted line in Fig. 4b (y=x-8) fits closely the number of misses in agreement with the asymptotic behavior showed by the hits. Meanwhile, the number of false positives also increased with the number of units present in the simulation, but it remained below 3. These results indicate that the decrease in detection performance was due to the grouping two or more neurons into single clusters, as exemplified in Fig. 3.

# 3.4. Sparse neurons

To quantify the spike sorting performance for different types of neurons, we divided our data into low- and high-firing neurons (see Section 2). Fig. 5a shows the hit ratio for both types of neurons and Fig. 5b and c the number of misses and false positives respectively. It can be seen that the performance for high-firing neurons was better than for the low-firing ones. For the cases with

**Table 1**Correct detections (Hits). Minimum, maximum and average number of hits for the 3 experts. The left column indexes the results by the number of units present in the simulation. Performances for the 3 experts were very similar. The last three columns display the global statistics, averaging across the 3 subjects.

Neurons	Operator 1			Operator 2			Operator 3			Total		
	Mean	Min	Max	Mean	Min	Max	Mean	Min	Max	Mean	Min	Max
2	1.8	1	2	1.8	1	2	1.8	1	2	1.8	1	2
3	2.8	2	3	2.8	2	3	2.8	2	3	2.8	2	3
4	3.8	3	4	3.6	3	4	3.6	3	4	3.67	3	4
5	4.2	3	5	3.8	2	5	4.4	3	5	4.13	2	5
6	5.2	4	6	5.2	5	6	5.2	5	6	5.2	4	6
7	5	3	7	4.6	2	6	4.8	2	7	4.8	2	7
8	6.8	6	7	6.6	6	7	6.2	6	7	6.53	6	7
9	7.2	5	8	6.8	5	8	7	4	9	7	4	9
10	6.4	3	9	6.2	4	9	6.6	5	8	6.4	3	9
11	8	6	9	7.8	6	10	7.6	6	9	7.8	6	10
12	8.4	7	11	7.2	6	9	7.2	6	9	7.6	6	11
13	8.6	5	11	8.2	3	11	7	3	9	7.93	3	11
14	7	5	11	7.2	4	11	6.6	4	11	6.93	4	11
15	8.2	6	11	7.8	5	10	7.8	5	10	7.93	5	11
16	10.6	10	11	9.6	8	11	10.8	9	12	10.33	8	12
17	7.4	5	9	5.8	5	7	6.4	4	8	6.53	4	9
18	9.2	6	12	9.2	6	13	7.4	4	12	8.6	4	13
19	8.4	6	11	8.2	5	11	6.4	5	8	7.66	5	11
20	9.4	7	12	7.8	5	11	7.8	5	11	8.33	5	12

**Table 2**False positives. Minimum, maximum and average false positives for the 3 experts. The left column indexes the results by the number of units present in the simulation. As in Table 1 results for different experts were very similar. The last three columns display the global statistics, averaging across the 3 subjects.

Neurons	Operator 1			Operator 2			Operator 3			Total		
	Mean	Min	Max	Mean	Min	Max	Mean	Min	Max	Mean	Min	Max
2	0.2	0	1	0	0	0	0.2	0	1	0.13	0	1
3	0	0	0	0	0	0	0.2	0	1	0.07	0	1
4	0	0	0	0	0	0	0	0	0	0	0	0
5	0.4	0	1	0.4	0	1	0.2	0	1	0.33	0	1
6	0	0	0	0	0	0	0.2	0	1	0.07	0	1
7	0.6	0	2	0.6	0	2	0.6	0	2	0.6	0	2
8	0.4	0	1	0.2	0	1	0.6	0	1	0.4	0	1
9	0.4	0	1	0.6	0	1	0.8	0	1	0.6	0	1
10	0.6	0	1	0.4	0	1	0.4	0	1	0.47	0	1
11	0.4	0	2	0.2	0	1	0.2	0	1	0.27	0	1
12	0.8	0	1	1.2	1	2	1.4	1	2	1.13	0	2
13	0.8	0	2	1	0	3	1.2	0	3	1	0	3
14	1.8	1	3	1.8	0	3	2.4	0	4	2	0	4
15	1.6	0	3	1.4	0	2	1.2	0	2	1.4	0	3
16	0.8	0	1	1.2	1	2	0.4	0	1	0.8	0	2
17	2.6	2	4	3.4	2	4	2.8	2	4	2.93	2	4
18	2.4	2	3	1.6	0	2	2.2	2	3	2.07	0	3
19	2.4	1	3	2	1	4	2.8	2	4	2.4	1	4
20	2.2	1	3	2.6	1	4	2.8	2	4	2.53	1	4

a large number of neurons, the ratio of misses for the low-firing neurons was around 80%, while for the high-firing neurons it reached values around 50%. These differences were statistically significant  $(F(1,511)=104.08, p<10^{-15}, F(1,511)=129.76, p<10^{-15}, Test 1, for hits and false positives, respectively). These results show the tendency of sparse neurons to be masked by multiunit activity or by cells with high firing rates.$ 

#### 4. Discussion

Recent studies have drawn attention to the apparent discrepancy between the number of neurons one expects to see following anatomical and physiological considerations – in the order of few hundred – and the number of neurons typically detected in experimental conditions with single electrodes – up to 6 – (Buzsaki, 2004; Shoham et al., 2006). This difference has been commonly attributed to the sparseness of neural firing (Henze et al., 2000; Olshausen and Field, 2004; Shoham et al., 2006; Fujisawa et al., 2008) and the damage of the neurological tissue around the electrode (Claverol-Tinture and Nadasdy, 2004). In addition to these factors, here we

showed that limitations of spike sorting algorithms also contribute to the relative low number of detected neurons.

#### 4.1. Limitations of spike sorting algorithms

Previous studies have analyzed and characterized the performance of several spike sorting methods (Letelier and Weber, 2000; Pouzat et al., 2002; Quian Quiroga et al., 2004; Zhang et al., 2004; Rutishauser et al., 2006; Vargas-Irwin and Donoghue, 2007). All these studies have, however, used relatively few neurons, thus not exploring the limits of spike sorting algorithms. Here we showed that the number of identified neurons reached a maximum of about 8–10, even when up to 20 neurons were present in the signal. Interestingly, there were relatively few false positives. Hence, the sorting mistakes were mainly produced by grouping 2 or more neurons into a single cluster, an effect also observed in previous studies but with a lower number of units (Blanche et al., 2005; Kwon et al., 2012). In addition, to show that this limitation of spike sorting is not exclusive of our own algorithm (Wave\_clus), we analyzed the same set of simulations using a completely different and well-known algo-

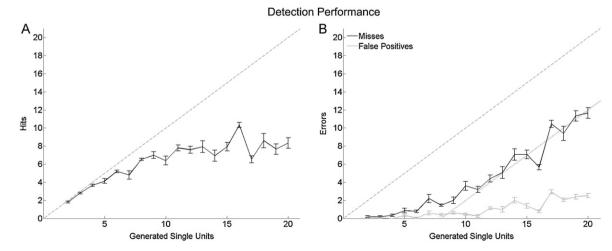
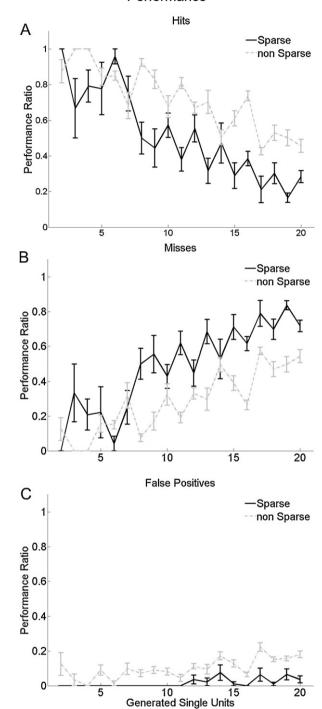


Fig. 4. Spike sorting performance with increasing number of neurons. The mean detection performance is shown as a function of the number of single units present in the simulation. (A) Average number of hits. (B) Average number of misses (black) and false positives (dashed gray). For the misses, the dotted gray line in B shows the linear function y = x - 8; i.e. a line parallel to the diagonal but displaced 8, the maximum number of neurons detected. Bars denote s.e.m.

# Sparse and non Sparse Neurons Performance



**Fig. 5.** Hits and false positive ratios for the sparse and non-sparse neurons. (A) Number of hits for sparse (dark gray) and non-sparse neurons (light gray), Number of misses (B) and false positives (C) for the same groups. Bars denote s.e.m.

rithm, KlustaKwik (Harris et al., 2000), and obtained very similar results to the ones presented here.

#### 4.2. Sparsely firing neurons

Our simulations included single units with a wide range of firing rates, as reported in experimental recordings (Musallam et al., 2004; Quian Quiroga et al., 2005; Fujisawa et al., 2008). The sorting

results for low- and high-firing neurons were significantly different and showed a better performance for the latter (see Fig. 5), despite the reported ability of the used algorithm to identify sparsely firing neurons in real recordings (Quian Quiroga et al., 2005, 2007, 2008). This is due to the fact that the activity of sparsely firing units is typically masked by the activity of neurons with higher firing rates recorded from the same channel. In other words, sparsely firing neurons show clusters with relatively few spikes which are typically merged with larger close-by clusters. A possible improvement could be to implement an iterative procedure to sort the remaining spikes after eliminating already identified (and large) clusters (Ott et al., 2005). However, the success of this approach is not guaranteed because the eliminated clusters could already include the activity of the sparsely firing neurons.

It has been reported that firing rates can be even lower (<0.05 spikes/s) than the ones we used in our simulations (Olshausen and Field, 2004; Shoham et al., 2006). Given the problem in detecting sparsely firing neurons described above, the presence of neurons with such low probability of firing would likely exacerbate even further the limitation of spike sorting algorithms, thus highlighting the difficulty of detecting this type of neurons, in line with previous studies (Henze et al., 2000; Buzsaki, 2004; Shoham et al., 2006; Fujisawa et al., 2008). This limitation is important because sparsely firing neurons have been related to high level cognitive processes (Quian Quiroga et al., 2008; Quian Quiroga, 2012), processing of sensory inputs (Olshausen and Field, 2004) and have been found all over the neocortex (Kerr et al., 2005; Shoham et al., 2006). Moreover, sparsely firing neurons usually carry high amounts of information per spike (Quian Quiroga et al., 2007; Quian Quiroga and Panzeri, 2009) and their responses can be strikingly selective (Quian Quiroga et al., 2007), show invariance (Quian Quiroga et al., 2005) and multimodality (Quian Quiroga et al., 2009). Furthermore, it has been shown that the bursting of a single neuron can modify the global brain state (Li et al., 2009) or even the behavior of an animal (Brecht et al., 2004; Houweling and Brecht, 2008). Altogether, these results highlight the need for further improvements of the spike sorting methods presently available, paying special attention to their performance with sparsely firing neurons.

#### 4.3. Tetrodes and stereotrodes

To improve the number of recorded units, a series of studies have proposed the transition from single electrode recordings to the use of tetrodes or stereotrodes (Gray et al., 1995; Harris et al., 2000; Blanche et al., 2005). These probes provide additional information by recording the firing of the neurons from different points (Harris et al., 2000) and they have been shown to provide better clustering outcomes (Gray et al., 1995; Harris et al., 2000). In our simulations we have only explored spike sorting limitations for single channel recordings. It is likely that with tetrodes the spike sorting algorithms would still identify a much lower number of neurons than the ones actually present in the recording, especially considering that with a tetrode it is possible to identify up to about 20 neurons in an area enclosing over 100 (Buzsaki, 2004). Interestingly, in a recording of cortical neurons in vivo using a 54 contact probe (Blanche et al., 2005), a comparison between sorting performances for a virtual tetrode (using only 4 adjacent contacts of the probe) and using a larger number of contacts showed that, in the case of the tetrode, 8 single units were identified, whereas when using the signal from all channels, 10 units were found: 7 corresponding to the ones found using the tetrode configuration and another 3 that were considered only one in the previous case. Interestingly, this particular error with the tetrode data - merging different single units into a same cluster - resembles the error described in Fig. 3 of our study.

The spike sorting process is determined by the shape and variance of the spikes, particularly the ones of neurons with the highest firing rates (contributing most of the spikes in a recording). This is related to the feature extraction phase of the algorithms, when the spikes are characterized in a feature space for posterior classification. The selected features reflect the main differences, which are determined by the large bulk of spikes of the high-firing neurons, and in turn, the features representing the spikes of the low-firing neurons tend to be underrepresented. In general, and beyond the particular issue of spike sorting, the clustering of groups with very different sizes is a known clustering problem (Ott et al., 2005).

The development of new recording probes that, for example, improve the quality of the signal transference from the tissue to the electrode and reduce the noise present in the signal (Keefer et al., 2008), opens the opportunity to dramatically increase the number of identified neurons from extracellular recordings. These developments should, however, be matched by advances in the methods used to process the recorded data. In this respect, the results presented here uncover the necessity of further improvement of spike sorting algorithms, particularly for the detection of sparsely firing neurons, as they are easily masked by neurons.

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#### Appendix A. Supplementary data

Supplementary data associated with this article can be found, in the online version, at http://dx.doi.org/10.1016/j.jneumeth.2012.07.010.

# References

- Blanche TJ, Spacek MA, Hetke JF, Swindale NV. Polytrodes: high-density silicon electrode arrays for large-scale multiunit recording. J Neurophysiol 2005:93:2987–3000.
- Brecht M, Schneider M, Sakmann B, Margie TW. Whisker movements evoked by stimulation of single pyramidal cells in rat motor cortex. Nature 2004;427:704–10.
- Brown EN, Kass RE, Mitra PP. Multiple neural spike train data analysis: state-of-theart and future challenges. Nat Neurosci 2004;7:456-61.
- Buzsaki G. Large-scale recording of neuronal ensembles. Nat Neurosci 2004;7:446-51.
- Carmena JM, Lebedev MA, Crist RE, O'Doherty JE, Santucci DM, Dimitrov DF, et al. Learning to control a brain-machine interface for reaching and grasping by primates. PLoS Biol 2003:1.
- Chapin JK. Using multi-neuron population recordings for neural prosthetics. Nat Neurosci 2004;7:452–5.
- Claverol-Tinture E, Nadasdy Z. Intersection of microwire electrodes with proximal CA1 stratum-pyramidale neurons at insertion for multiunit recordings predicted by a 3-D computer model. IEEE Trans Biomed Eng 2004;51:2211–6.
- Donoghue JP. Connecting cortex to machines: recent advances in brain interfaces. Nat Neurosci 2002;5:1085–8.
- Douglas RJ, Martin KAC. Opening the grey box. Trends Neurosci 1991;14:286–93. Fujisawa S, Amarasingham A, Harrison MT, Buzsáki G. Behavior-dependent short-term assembly dynamics in the medial prefrontal cortex. Nat Neurosci
- 2008;11:823–33. Gold C, Henze DA, Koch C, Buzsaki G. On the origin of the extracellular action potential waveform: a modeling study. J Neurophysiol 2006;95:3113–28.
- Gray CM, Maldonado PE, Wilson M, McNaughton B. Tetrodes markedly improve the reliability and yield of multiple single-unit isolation from multi-unit recordings in cat striate cortex. J Neurosci Methods 1995;63:43–54.

- Harris KD, Csicsvari J, Hirase H, Dragoi G, Buzsaki G. Organization of cell assemblies in the hippocampus. Nature 2003;424:552-6.
- Harris KD, Henze DA, Csicsvari J, Hirase H, Buzsaki G. Accuracy of tetrode spike separation as determined by simultaneous intracellular and extracellular measurements. J Neurophysiol 2000;84:401–14.
- Henze DA, Borhegyi Z, Csicsvari J, Mamiya A, Harris KD, Buzsaki G. Intracellular features predicted by extracellular recordings in the hippocampus in vivo. J Neurophysiol 2000;84:390–400.
- Houweling AR, Brecht M. Behavioural report of single neuron stimulation in somatosensory cortex. Nature 2008;451:65–8.
- Jackson A, Fetz EE. Compact movable microwire array for long-term chronic unit recording in cerebral cortex of primates. J Neurophysiol 2007;98:3109-18.
- Keefer EW, Botterman BR, Romero MI, Rossi AF, Gross GW. Carbon nanotube coating improves neuronal recordings. Nat Nanotechnol 2008;3:434.
- Kerr JND, Greenberg D, Helmchen F. Imaging input and output of neocortical networks in vivo. Proc Natl Acad Sci USA 2005;102:14063–8.
- Kwon KY, Eldawlatly S, Oweiss K. NeuroQuest: a comprehensive analysis tool for extracellular neural ensemble recordings. J Neurosci Methods 2012;204:189–201.
- Letelier JC, Weber PP. Spike sorting based on discrete wavelet transform coefficients. J Neurosci Methods 2000;101:93–106.
- Li CY, Poo MM, Dan Y. Burst spiking of a single cortical neuron modifies global brain state. Science 2009;324:643–6.
- Martinez J, Pedreira C, Ison MJ, Quian Quiroga R. Realistic simulation of extracellular recordings. J Neurosci Methods 2009;184:285–93.
- Maynard EM, Nordhausen CT, Normann RA. The Utah Intracortical Electrode Array: a recording structure for potential brain-computer interfaces. Electroencephalogr Clin Neurophysiol 1997;102:228–39.
- Moffitt MA, McIntyre CC. Model-based analysis of cortical recording with silicon microelectrodes. Clin Neurophysiol 2005;116:2240–50.
- Musallam S, Corneil BD, Greger B, Scherberger H, Andersen RA. Cognitive control signals for neural prosthetics. Science 2004;305:258–62.
- Nicolelis MAL, Lebedev MA. Principles of neural ensemble physiology underlying the operation of brain-machine interfaces. Nat Rev Neurosci 2009;10: 530–40
- Olshausen BA, Field DJ. Sparse coding of sensory inputs. Curr Opin Neurobiol 2004:14:481-7.
- Ott T, Kern A, Steeb WH, Stoop R. Sequential clustering: tracking down the most natural clusters. J Stat Mech Theor Exp 2005;2005:P11014.
- Pouzat C, Mazor O, Laurent G. Using noise signature to optimize spike-sorting and to assess neuronal classification quality. J Neurosci Methods 2002;122:43–57.
- Quian Quiroga R. Concept cells: the building blocks of declarative memory functions. Nat Rev Neurosci 2012;13:587–97.
- Quian Quiroga R, Kraskov A, Koch C, Fried I. Explicit encoding of multimodal percepts by single neurons in the human brain. Curr Biol 2009: 19:1308–13.
- Quian Quiroga R, Kreiman G, Koch C, Fried I. Sparse but not 'Grandmother-cell' coding in the medial temporal lobe. Trends Cogn Sci 2008;12:87–91.
- Quian Quiroga R, Nadasdy Z, Ben-Shaul Y. Unsupervised spike detection and sorting with wavelets and super-paramagnetic clustering. Neural Comput 2004:16:1661-87.
- Quian Quiroga R, Panzeri S. Extracting information from neuronal populations: Information theory and decoding approaches. Nat Rev Neurosci 2009;10:173–85.
- Quian Quiroga R, Reddy L, Koch C, Fried I. Decoding Visual Inputs From Multiple Neurons in the Human Temporal Lobe. J Neurophysiol 2007;98:1997.
- Quian Quiroga R, Reddy L, Kreiman G, Koch C, Fried I. Invariant visual representation by single neurons in the human brain. Nature 2005;435:1102–7.
- Rutishauser U, Schuman EM, Mamelak AN. Online detection and sorting of extracellularly recorded action potentials in human medial temporal lobe recordings, in vivo. J Neurosci Methods 2006;154:204–24.
- Shoham S, O'Connor DH, Segev R. How silent is the brain: is there a "dark matter" problem in neuroscience? J Comp Physiol A Neuroethol Sens Neural Behav Physiol 2006:192:777–84.
- Tolias AS, Ecker AS, Siapas AG, Hoenselaar A, Keliris GA, Logothetis NK. Recording chronically from the same neurons in awake, behaving primates. J Neurophysiol 2007:98:3780–90.
- Vargas-Irwin C, Donoghue JP. Automated spike sorting using density grid contour clustering and subtractive waveform decomposition. J Neurosci Methods 2007;164:1–18.
- Velliste M, Perel S, Spalding MC, Whitford AS, Schwartz AB. Cortical control of a prosthetic arm for self-feeding. Nature 2008;453:1098–101.
- Wehr M, Pezaris JS, Sahani M. Simultaneous paired intracellular and tetrode recordings for evaluating the performance of spike sorting algorithms. Neurocomputing 1999:26–27:1061–8.
- Zhang PM, Wu JY, Zhou Y, Liang PJ, Yuan JQ. Spike sorting based on automatic template reconstruction with a partial solution to the overlapping problem. J Neurosci Methods 2004;135:55-65.