

Pape



Slides





# Plug-and-Play Priors for Reconstruction-based Placental Image Registration (PnP-RR)

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Paper



Slides





# **Brief Intro**

- We proposed plug-and-play reconstruction-registration method (PnP-RR):
  - 1) Is a deformable image registration framework for severely noise-corrupted images
  - 2) Is used for registering placental diffusion-weighted MR images that contains severely noise



**Paper** 



Slides





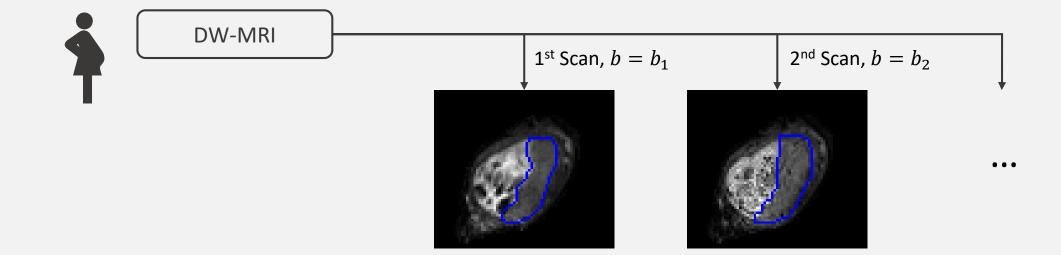
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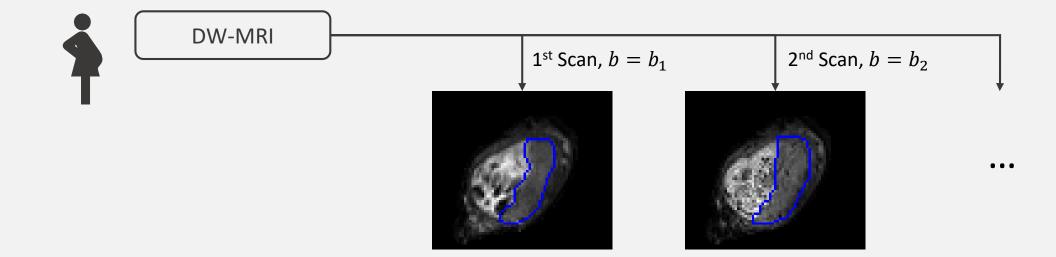
## **Contents**

- 1. Background
  - 1) DW-MRI
  - 2) Image registration
- 2. Related works
- 3. Proposed method: PnP-RR
- 4. Experiments and results
- 5. Discussion and conclusion

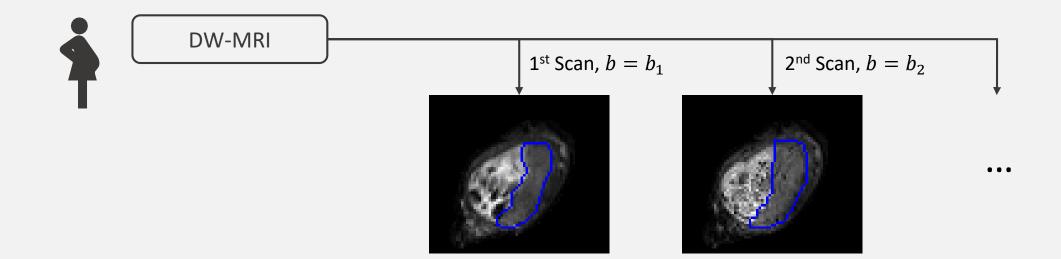
- Placenta and DW-MRI
  - Diffusion-weighted MRI (DW-MRI) for placental health monitoring



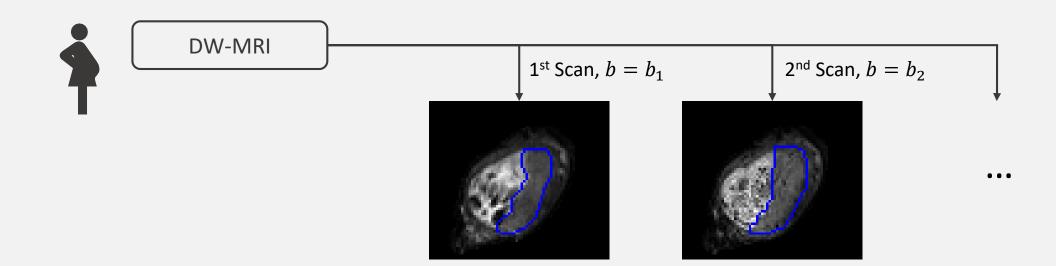
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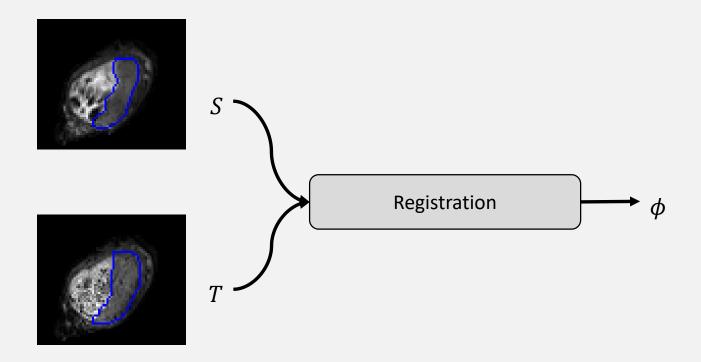
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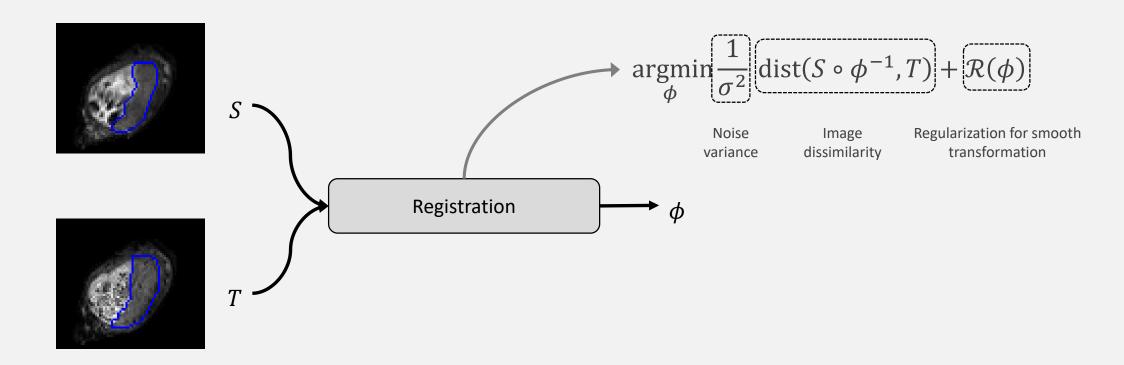
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  - Need Image registration to find and cancel the deformation



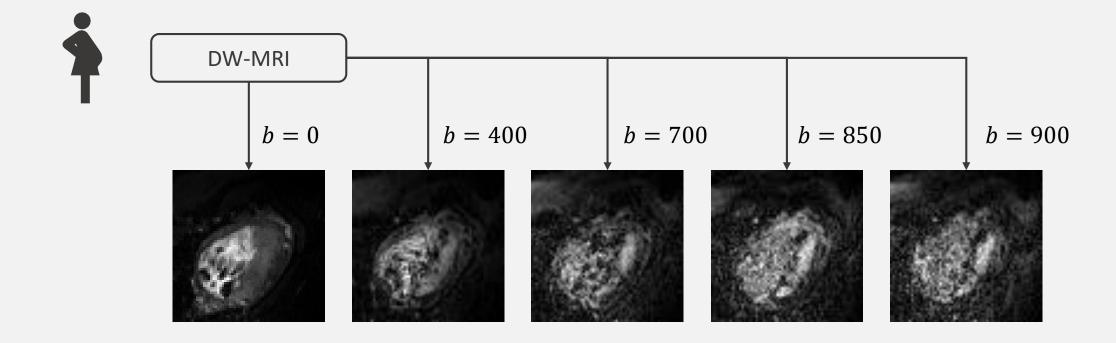
- Image Registration
  - Task: find the deformation  $\phi$  between a source Image S and a target image T



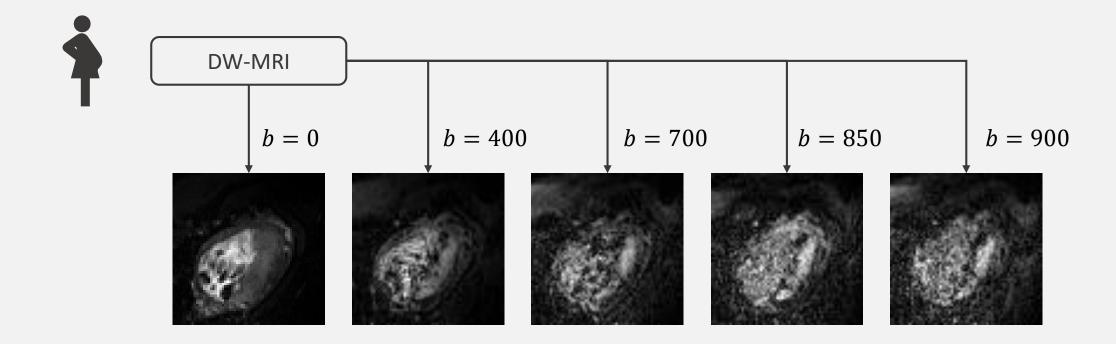
- Image Registration
  - Task: find the deformation  $\phi$  between a source Image S and a target image T
  - Current mainstream: optimization-based methods



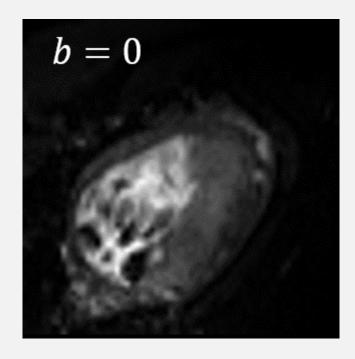
- B-value and noise
  - Higher b-value, stronger noise

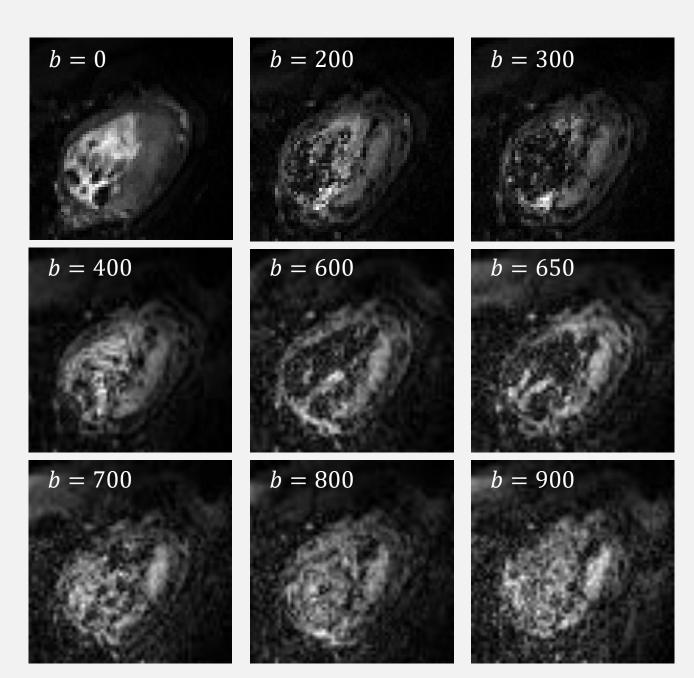


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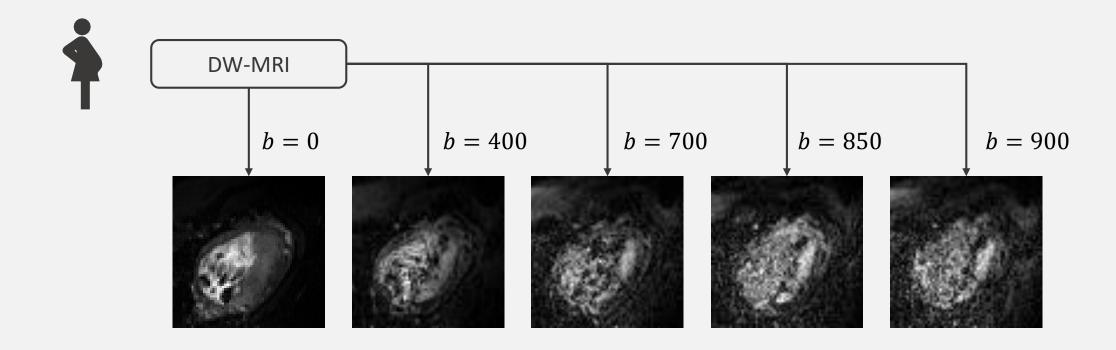


- B-value and noise
  - DW-MRI images with different b-values





- B-value and noise
  - Higher b-value, stronger noise
  - Ordinary registration methods: fail on severely noise-corrupted images
  - A noise-robust image registration methods is needed



- Basic idea: denoising + registration
  - Integrate image registration with denoising

- Basic idea: denoising + registration
  - Integrate image registration with denoising
  - Denoising example: total variation denoising for white Gaussian noise



Original

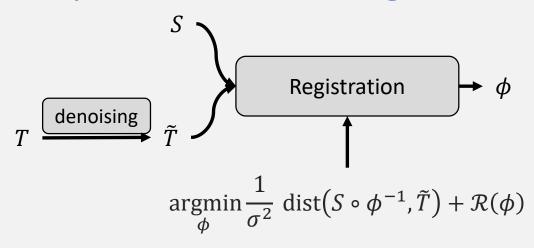


Noisy Image



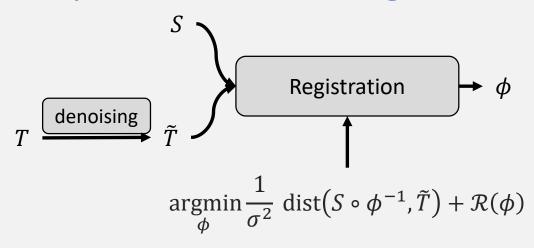
Denoised image

• 2-Steps Method: denoising before registration



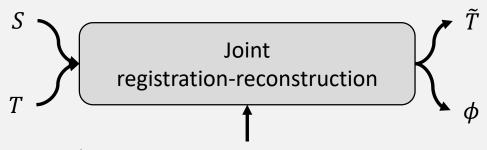
May **NOT** converge to **OPTIMAL** solution

• 2-Steps Method: denoising before registration



May **NOT** converge to **OPTIMAL** solution

Joint Optimization Method

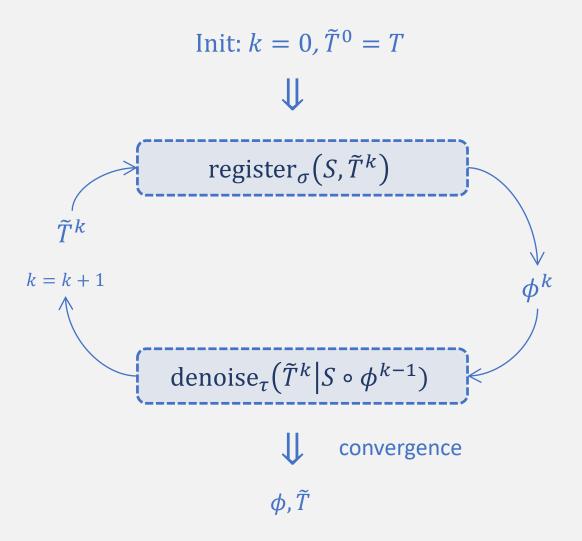


Requires explicit objective function;

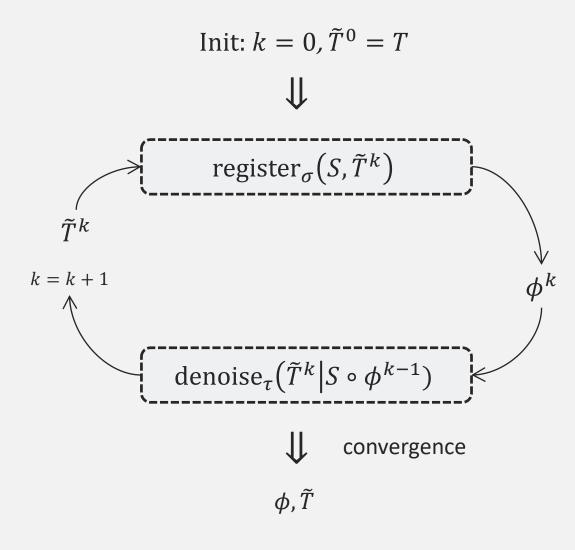
-> **LIMITED CHOICES** for denoisers

$$\underset{\phi,T}{\operatorname{argmin}} \frac{1}{\sigma^2} \operatorname{dist}(S \circ \phi^{-1}, T) + \mathcal{R}_{\operatorname{reg}}(\phi) + \lambda_1 R_{\operatorname{denoising}}(\tilde{T}) + \lambda_2 \operatorname{dist}(T, \tilde{T})$$

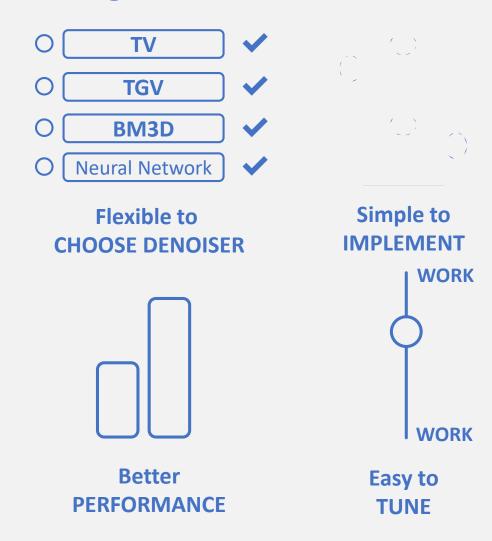
• Basic Idea



• Basic Idea



Advantages



- Derivation
  - JOINT denoising-registration objective function

$$\underset{\phi,\tilde{T}}{\operatorname{argmin}} \frac{1}{\sigma^2} \left\| S \circ \phi^{-1} - \tilde{T} \right\|_{L2}^2 + \mathcal{R}_{\operatorname{reg}}(\phi) + \lambda_1 \mathcal{R}_{\operatorname{denoising}}(\tilde{T}) + \lambda_2 \left\| T - \tilde{T} \right\|_{L2}^2$$

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SPLIT Formulated as proximal algorithm

$$\underset{\phi}{\operatorname{argmin}} \frac{1}{\sigma^2} \| S \circ \phi^{-1} - \tilde{T} \|_{L2}^2 + \mathcal{R}_{\operatorname{reg}}(\phi) = \operatorname{register}_{\sigma} (S, \tilde{T}^k)$$

$$\underset{\tilde{T}}{\operatorname{argmin}} \frac{1}{2} \| \tilde{T} - Z \|_{L2}^2 + \tau \mathcal{R}_{\operatorname{denoising}}(\tilde{T}) = \operatorname{denoise}_{\tau}(\tilde{T} | S \circ \phi^{-1}) \text{ where}$$

$$Z = \frac{\lambda_2 T + (1/\sigma^2)(S \circ \phi^{-1})}{\lambda_2 + (1/\sigma^2)}$$

$$\tau = \frac{\lambda_1}{2(\lambda_2 + (1/\sigma^2))}$$

- Derivation
  - JOINT denoising-registration objective function

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 acce with 
$$\operatorname{register}_{\sigma} \left( S, \tilde{T}^k \right)$$
 register 
$$(S, \tilde{T}^k)$$

Replace with arbitrary denoiser register  $(S, \tilde{T}^k)$  denoise  $(S, \tilde{T}^k)$ 

- Derivation
  - JOINT denoising-registration objective function

$$\underset{\phi,\tilde{T}}{\operatorname{argmin}} \frac{1}{\sigma^2} \left\| S \circ \phi^{-1} - \tilde{T} \right\|_{L^2}^2 + \mathcal{R}_{\operatorname{reg}}(\phi) + \left[ \lambda_1 \mathcal{R}_{\operatorname{denoising}}(\tilde{T}) + \lambda_2 \left\| T - \tilde{T} \right\|_{L^2}^2 \right] + C$$

SPLIT Formulated as proximal algorithm

$$\underset{\phi}{\operatorname{argmin}} \frac{1}{\sigma^{2}} \| S \circ \phi^{-1} - \tilde{T} \|_{L2}^{2} + \mathcal{R}_{\operatorname{reg}}(\phi) = \operatorname{register}_{\sigma} (S, \tilde{T}^{k})$$

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where

REPLACE Formulated as PnP algorithm

$$Z = \frac{\lambda_2 T + (1/\sigma^2)(S \circ \phi^{-1})}{\lambda_2 + (1/\sigma^2)}$$
$$\tau = \frac{\lambda_2 T + (1/\sigma^2)}{\lambda_1}$$

register<sub>$$\sigma$$</sub> (S,  $\tilde{T}^k$ )

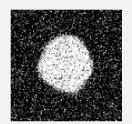
denoise 
$$_{\tau}(Z)$$

Specifying an image prior

- Data
  - 2D synthetic data

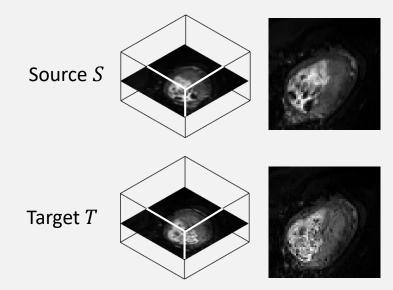






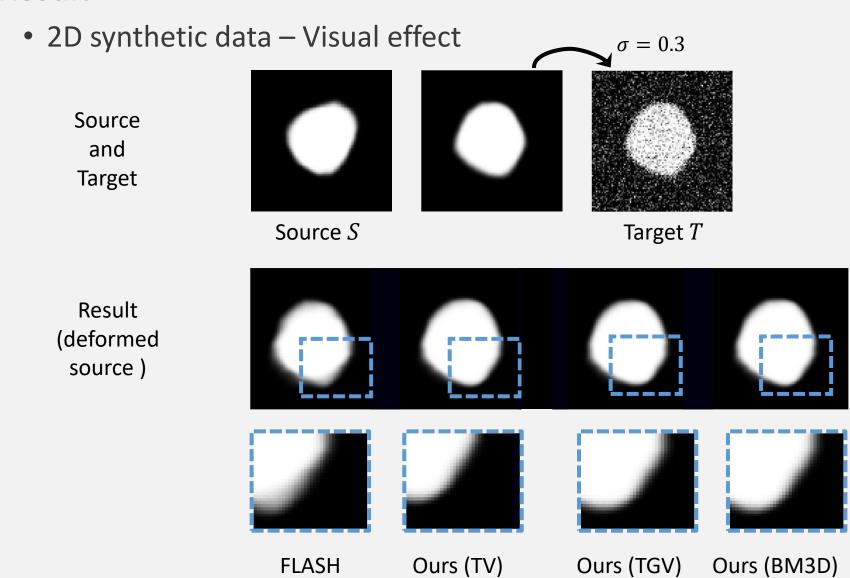
Target T

Real 3D DW-MRI data

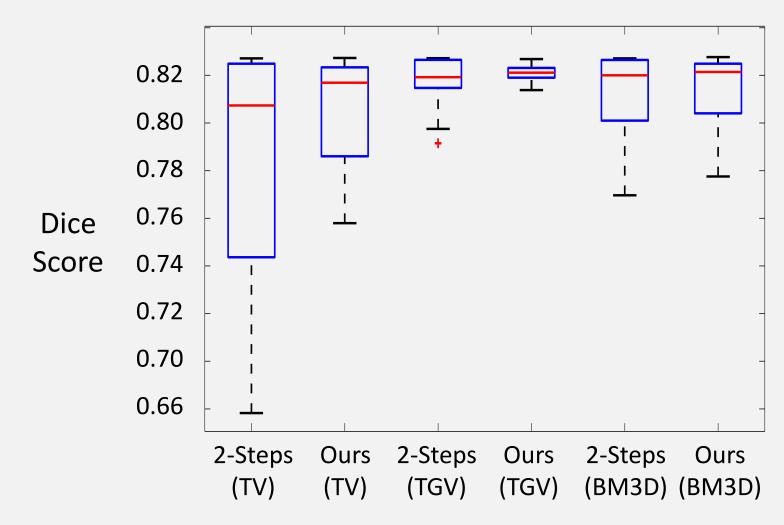


- Algorithm Setting
  - Registration algorithm
    - Fourier-approximated Lie Algebras for Shooting (FLASH)<sup>[1]</sup>
  - Denoising algorithm
    - Total variation (TV)
    - Total generalized variation (TGV)
    - Block-matching and 3D filtering (BM3D)

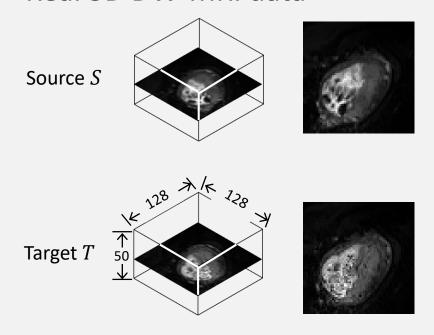
Result



- Result
  - 2D synthetic data Quantitative performance

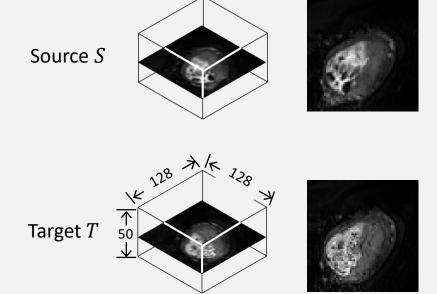


- Data
  - Real 3D DW-MRI data



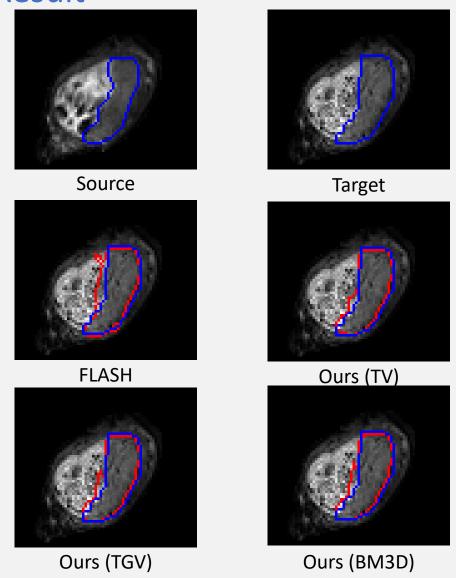
All DW-MRIs are of dimension 128 × 128 × 50 and underwent bias field correction, co-registration with affine transformations and intensity normalization

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#### Result



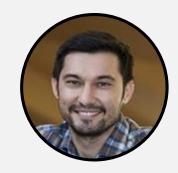
## **Discussion**

- Performance
  - Data
  - Advanced methods
- Convergence
- Time

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Miaomiao Zhang

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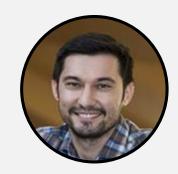


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- Questions?



Jiarui Xing



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