

# Change in Ultrasonic Backscattered Energy for Temperature Imaging: Factors Affecting Temperature Accuracy and Spatial Resolution in 3D

R. Martin Arthur<sup>1</sup>, Jason W. Trobaugh<sup>1</sup>,  
William L. Straube<sup>2</sup>, Yuzheng Guo<sup>1</sup>, and  
Eduardo G. Moros<sup>3</sup>

<sup>1</sup>Electrical & Systems Engineering

<sup>2</sup>Radiation Oncology

Washington University in St. Louis.

St. Louis, MO, 63130, USA

<sup>3</sup>Radiation Oncology, University of Arkansas

Supported by NIH Grants R21 CA90531, R01 CA107558 and the  
Wilkinson Trust at Washington University



Washington University in St. Louis

32<sup>nd</sup> UITC

Arlington, VA 5/16/07

# Objective of Ultrasonic Thermometry

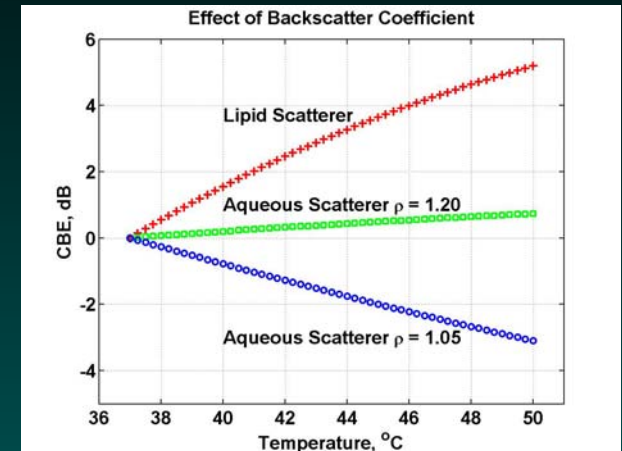
To develop a method to produce 3D temperature maps in soft tissue during hyperthermia cancer treatment

- with at least  $0.5^{\circ}\text{C}$  accuracy &  $1\text{ cm}^3$  resolution
- non-invasively, conveniently at low cost with a single view from standard equipment

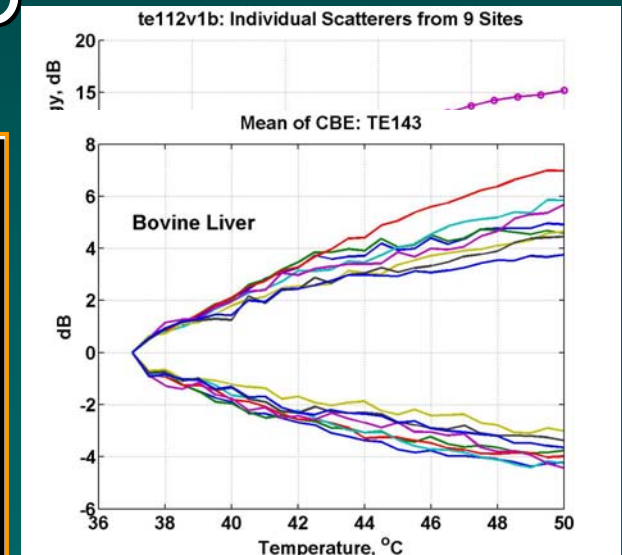
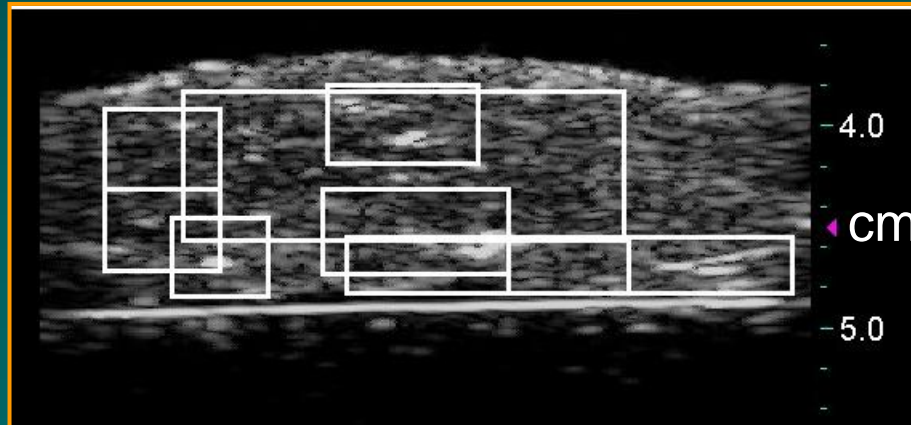


# Change in backscattered energy (CBE) as a monotonic temperature-dependent parameter

- CBE single-scatterer prediction  
*U Med & Bio, 20:915-922, 1994*
- CBE from isolated echoes in 1D  
*Medical Physics, 30:1021-1029, 2003*
- CBE over selected regions in 2D  
*IEEE UFFC, 52:1644-1652, 2005*



Bovine  
Liver



# I. Simulation of Scatterer Collections

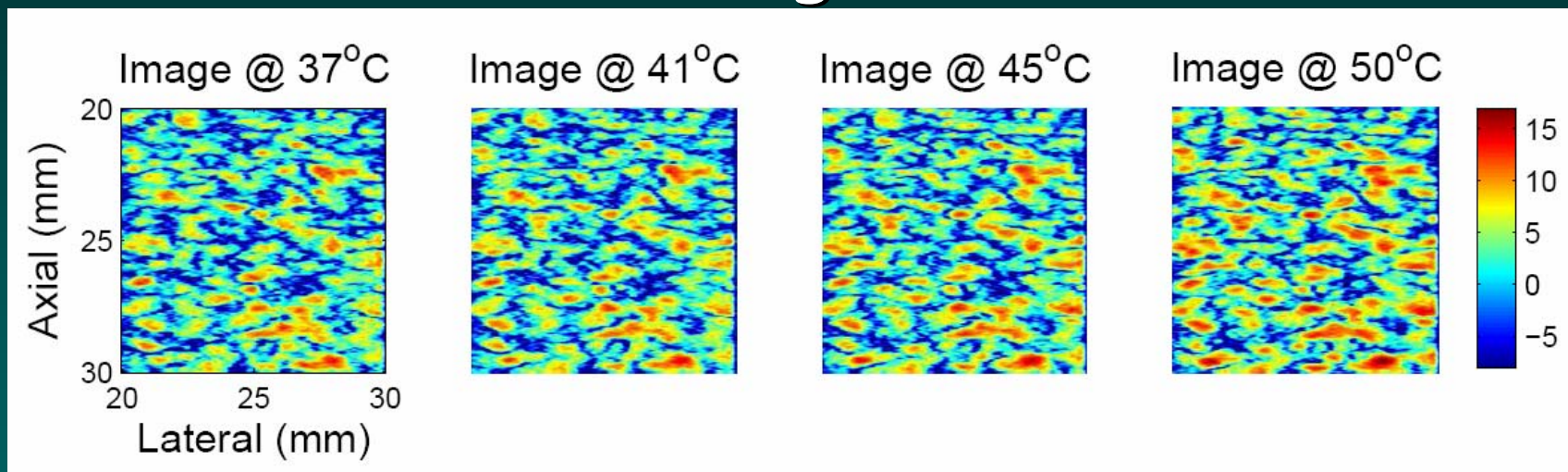
- To provide a theoretical representation for images of multiple scatterers to extend our single-scatterer model
- To determine limits on spatial resolution and temperature accuracy by studying effects of
  - Scatterer Population
  - Signal-to-Noise Ratio
  - Region Size



# Simulation Methods

## Discrete-Scatterer Model

- Superposition of point-spread-functions
- Temperature dependence of individual scatterers from single-scatterer model



Simulated images for heating of lipid and aqueous scatterers randomly placed in a liver-like medium



Trobaugh & Arthur, *IEEE Trans. UFFC*, 48:1594-1605, 2001

Trobaugh et al., *Ultrasound in Med. & Biol.*, in review

Washington University in St. Louis

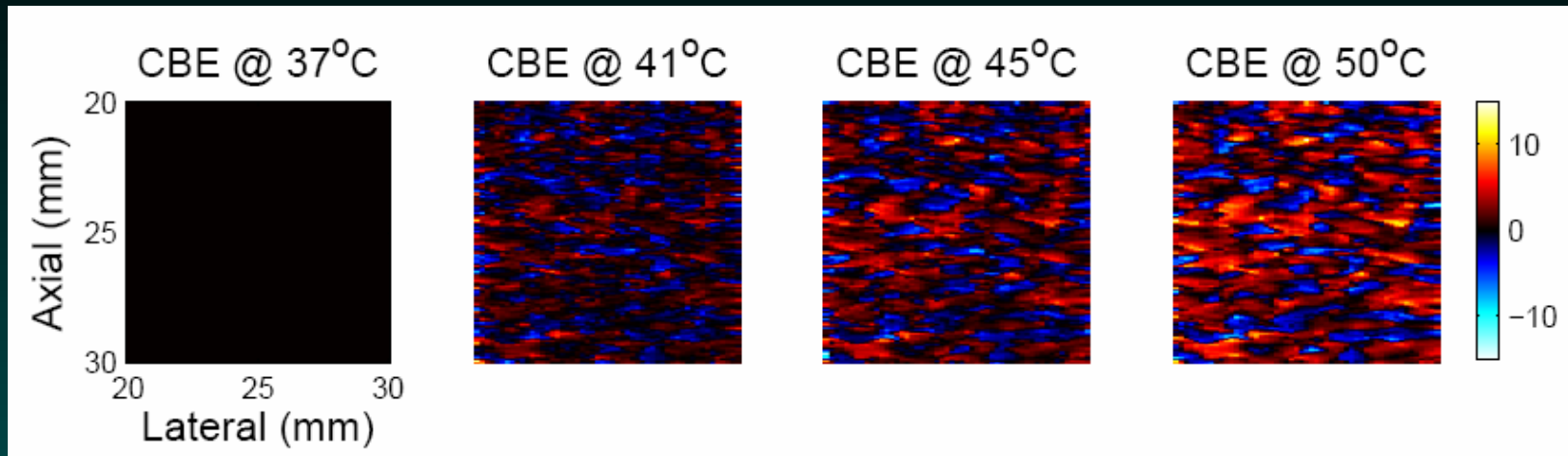
R. M. Arthur 5 of 20

32<sup>nd</sup> UITC

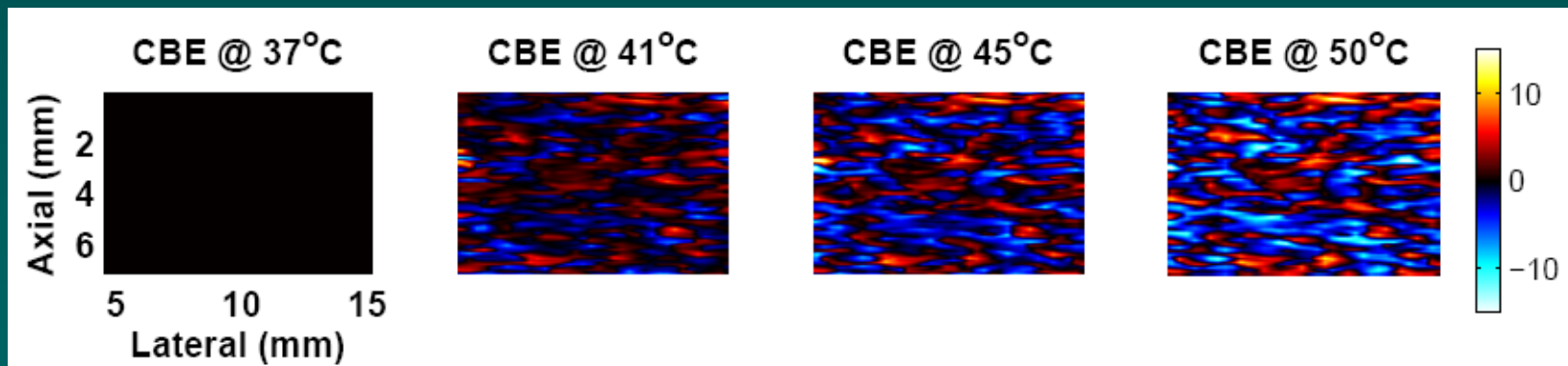
Arlington, VA 5/16/07



# Simulated and Measured CBE



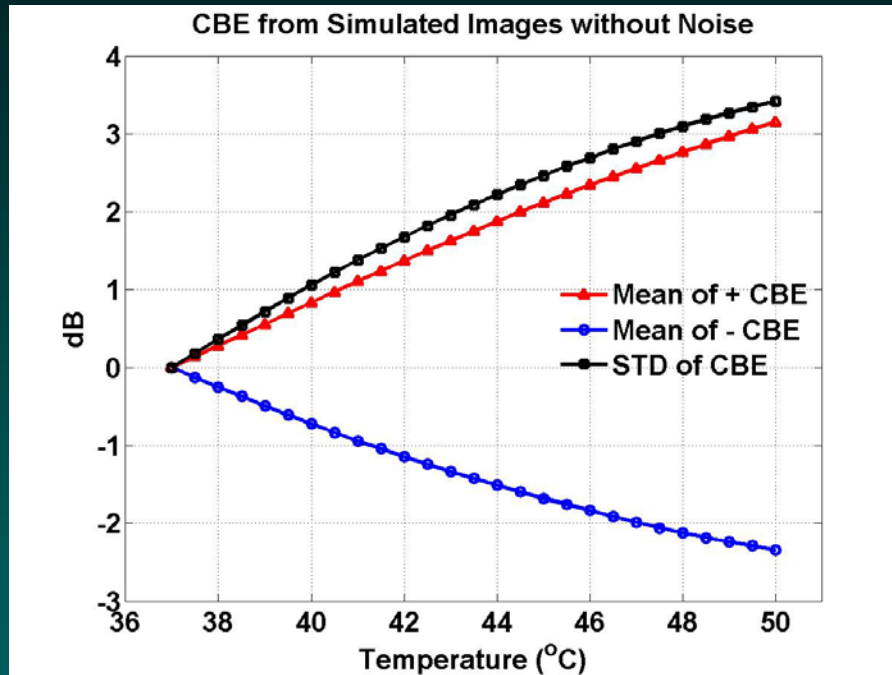
CBE from simulated images computed in the same manner used for measured images  
Increase in BE (red) Decrease in BE (blue)



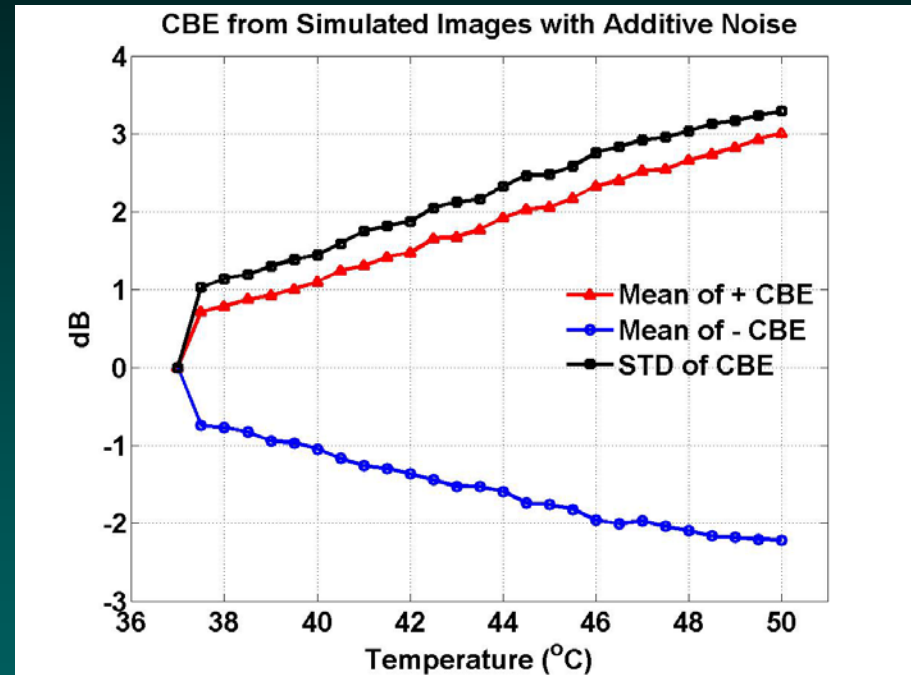
CBE measured in bovine liver



# Change in Backscattered Energy from Simulated Images



No Noise

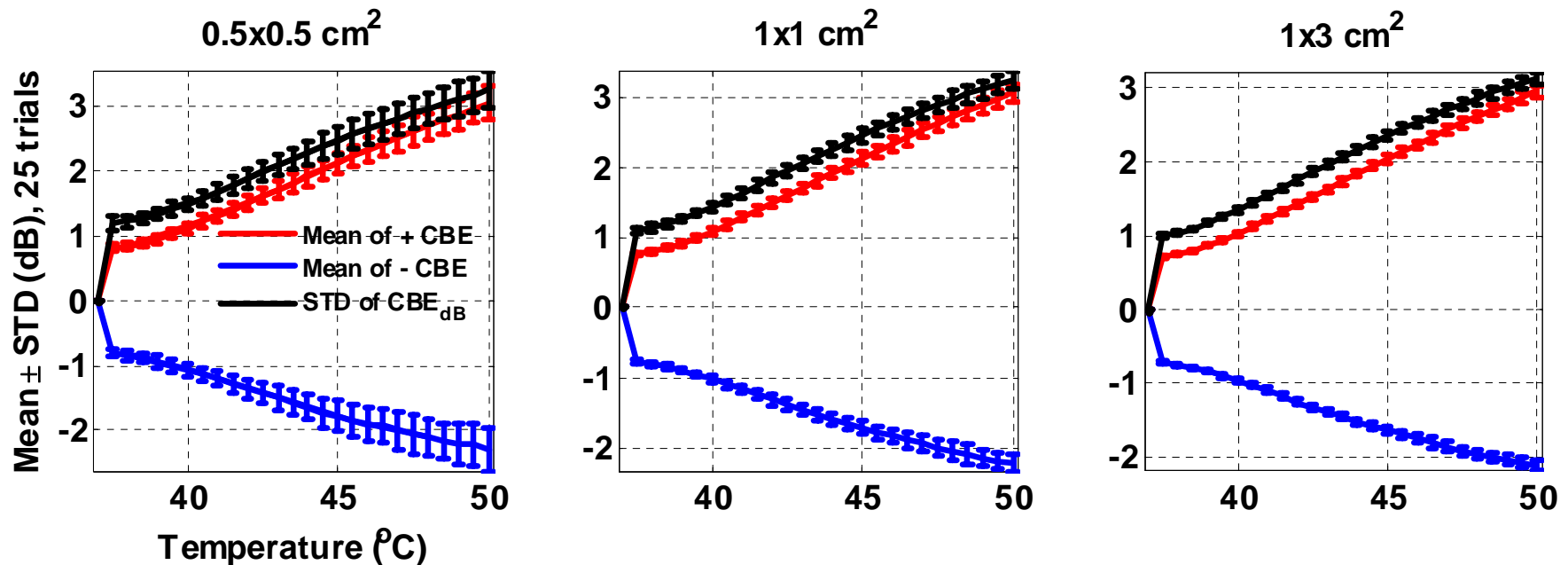


With Noise (SNR=19dB)

Multiple sub-wavelength scatterers  
(2:1 ratio of lipid to aqueous scatterers)



# Change in Backscattered Energy from Simulated Images

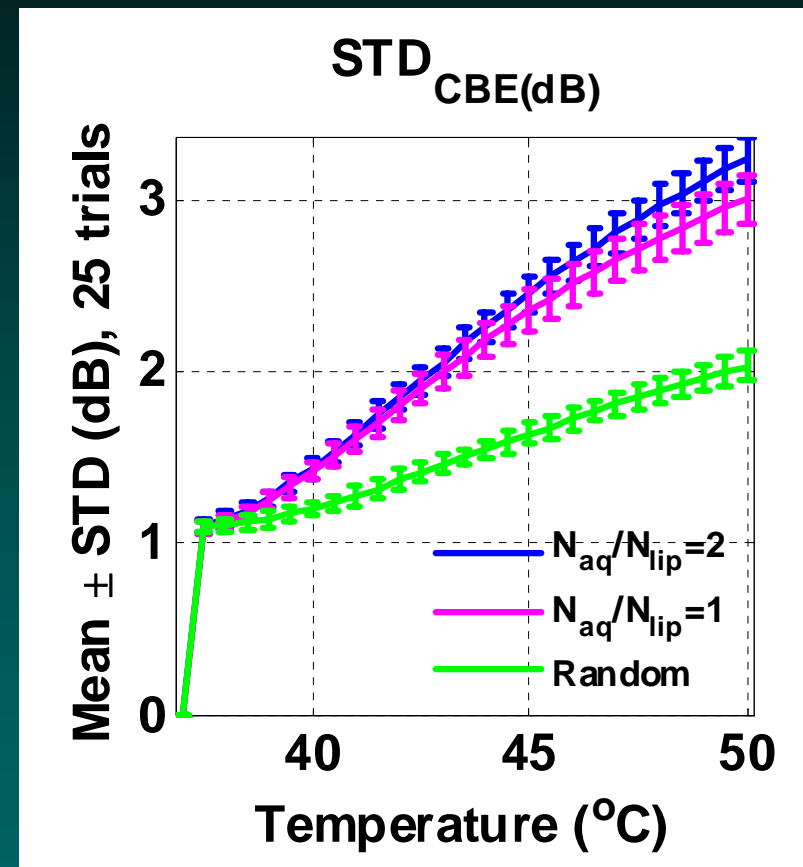
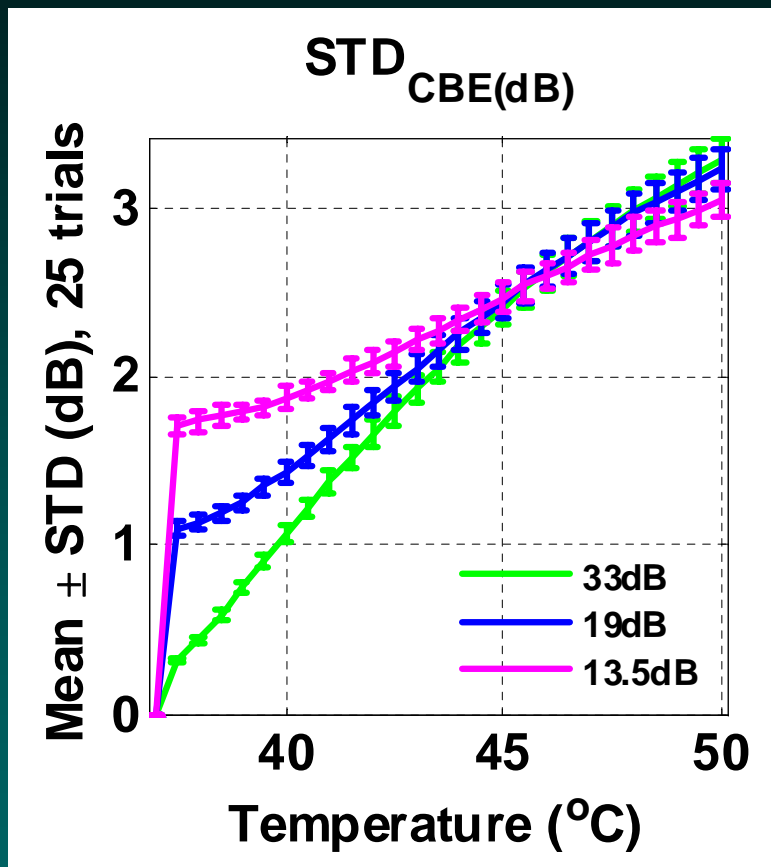


Region Size





# Change in Backscattered Energy from Simulated Images



Signal-to-Noise

Scatterer Population

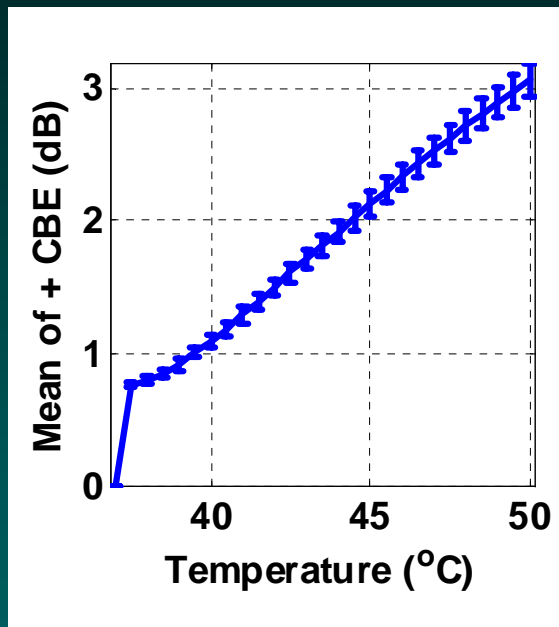


Washington University in St. Louis

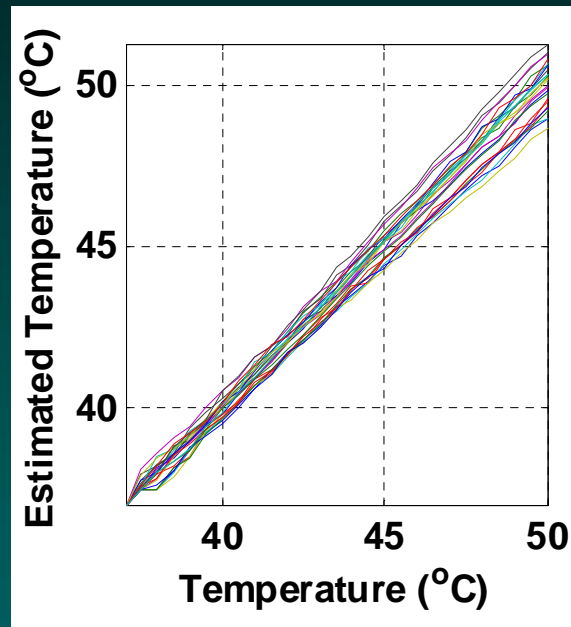
R. M. Arthur 9 of 20

32<sup>nd</sup> UITC  
Arlington, VA 5/16/07

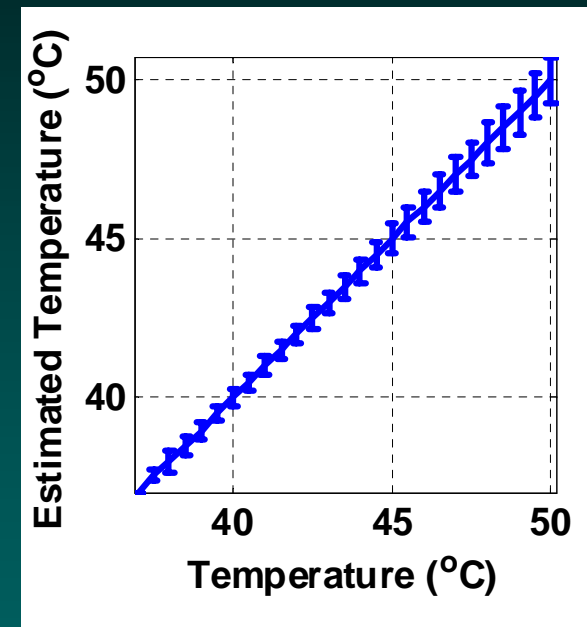
# Temperature Estimation from CBE in Simulated Images



Calibration



Estimates



Errors



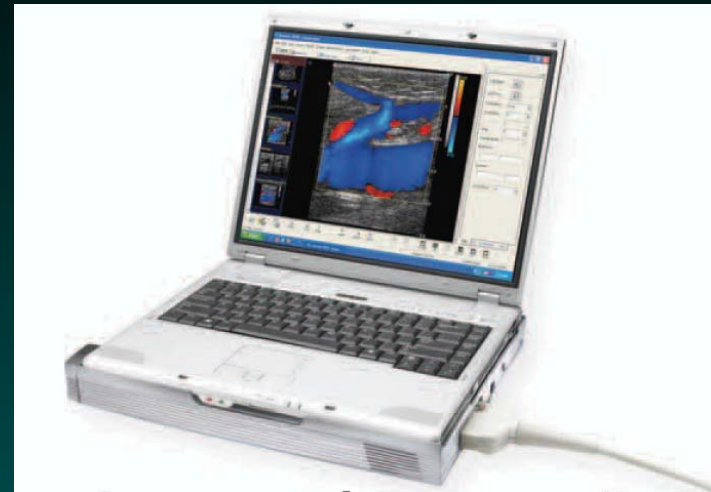
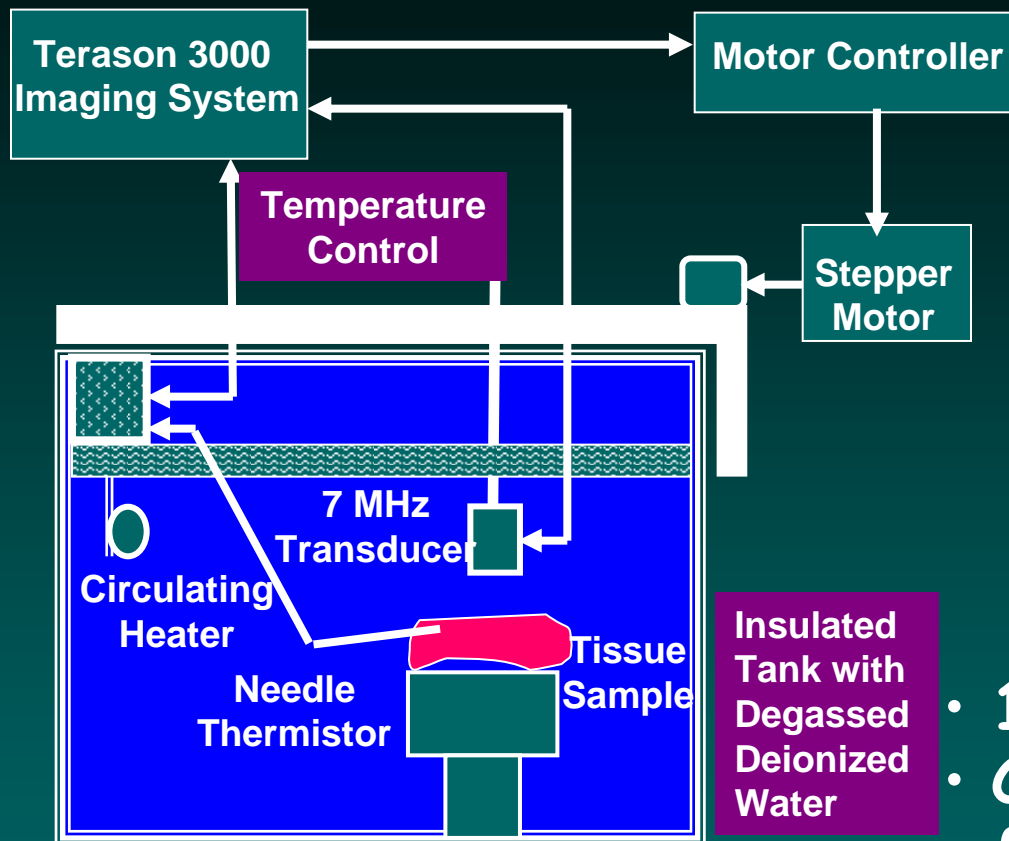
# Temperature Estimation from CBE in Simulated Images

	Mean + CBE	Mean - CBE	STD CBE
Scatterer Population	Accuracy ( $\pm^\circ\text{C}$ )	Accuracy ( $\pm^\circ\text{C}$ )	Accuracy ( $\pm^\circ\text{C}$ )
$N_{aq}/N_{lip} = 2$ (baseline)	0.716	1.385	0.971
$N_{aq}/N_{lip} = 1$	0.897	1.649	1.116
Random f(T)	0.612	2.222	1.227
Signal-to-Noise Ratio			
13.5dB	0.917	1.839	1.175
19dB (baseline)	0.716	1.385	0.971
33dB	0.907	1.144	0.768
Region Size ( $\text{cm}^2$ )			
.5x.5	1.485	2.291	1.817
1x1 (baseline)	0.716	1.385	0.971
1x3	0.488	0.768	0.583

Accuracy (95%) in  $^\circ\text{C}$  for  
estimating temperature at  $44^\circ\text{C}$



## II. Temperature Estimation *in vitro*



Terason 3000 (Teratech, Corp., Burlington, MA)

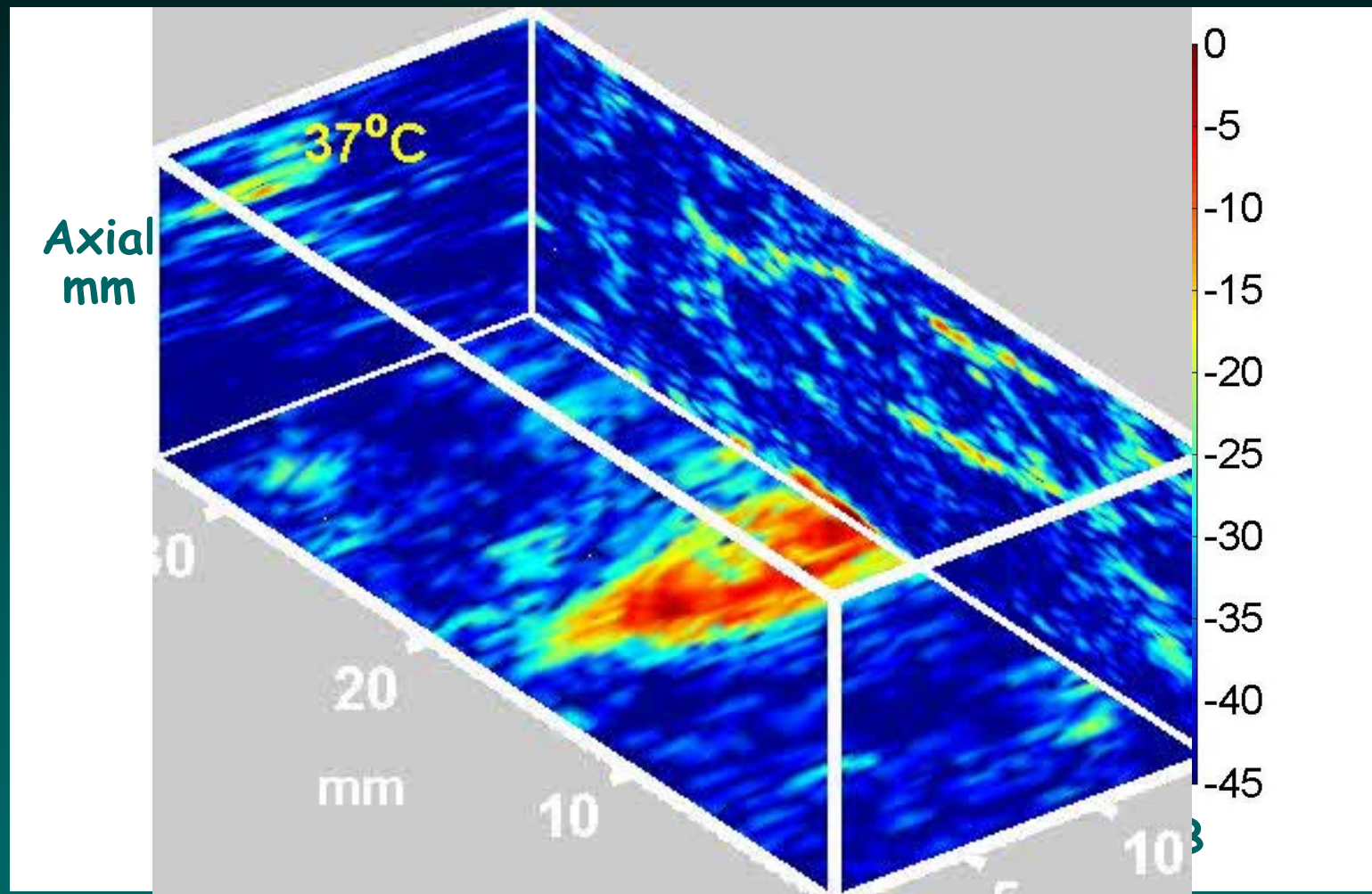
- 128 Element 7 MHz Array
- Control of temperature from 37 to 50°C and image acquisition with AutoIt®
- Access to RF signals

### 3D Dataset

Images were taken at 0.6 mm intervals in elevation at each temperature

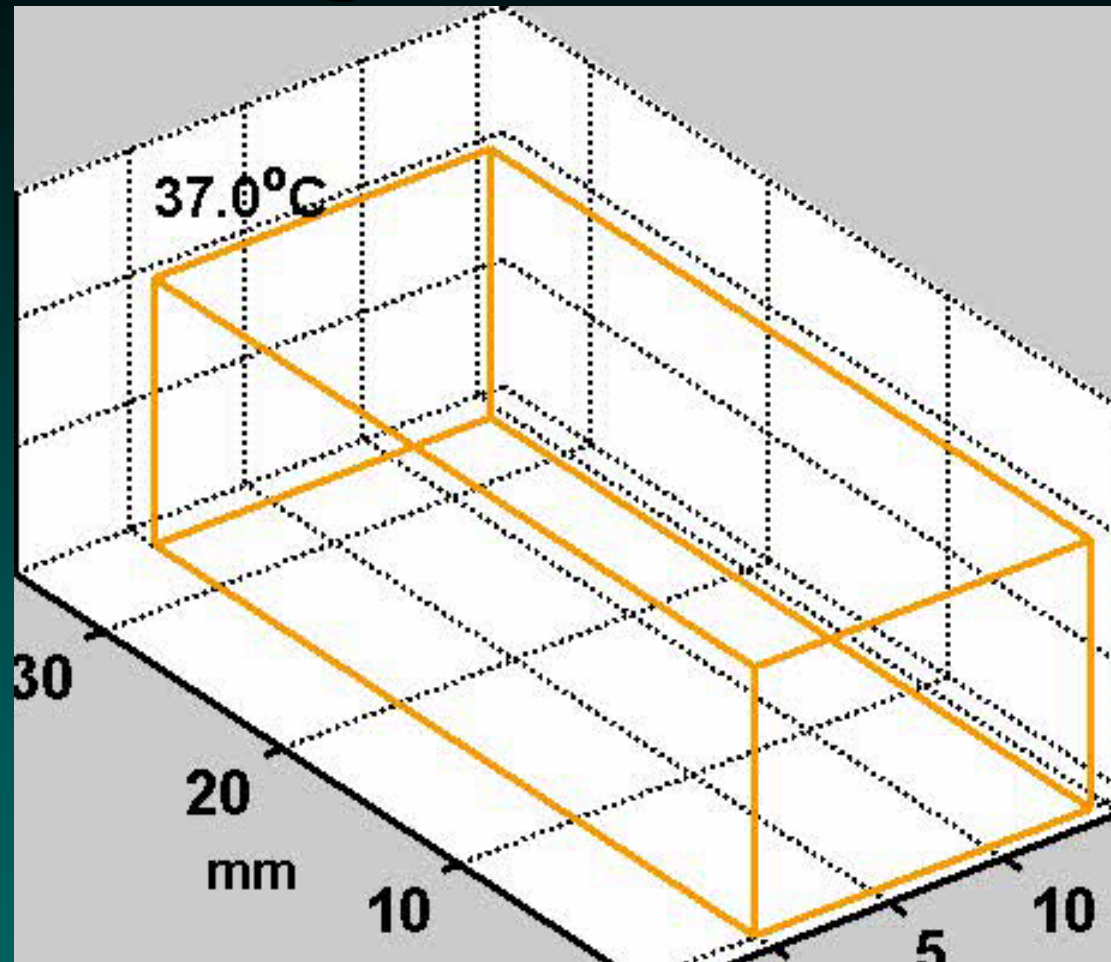


# Measured Backscattered Images in 3D from 37 to 50°C





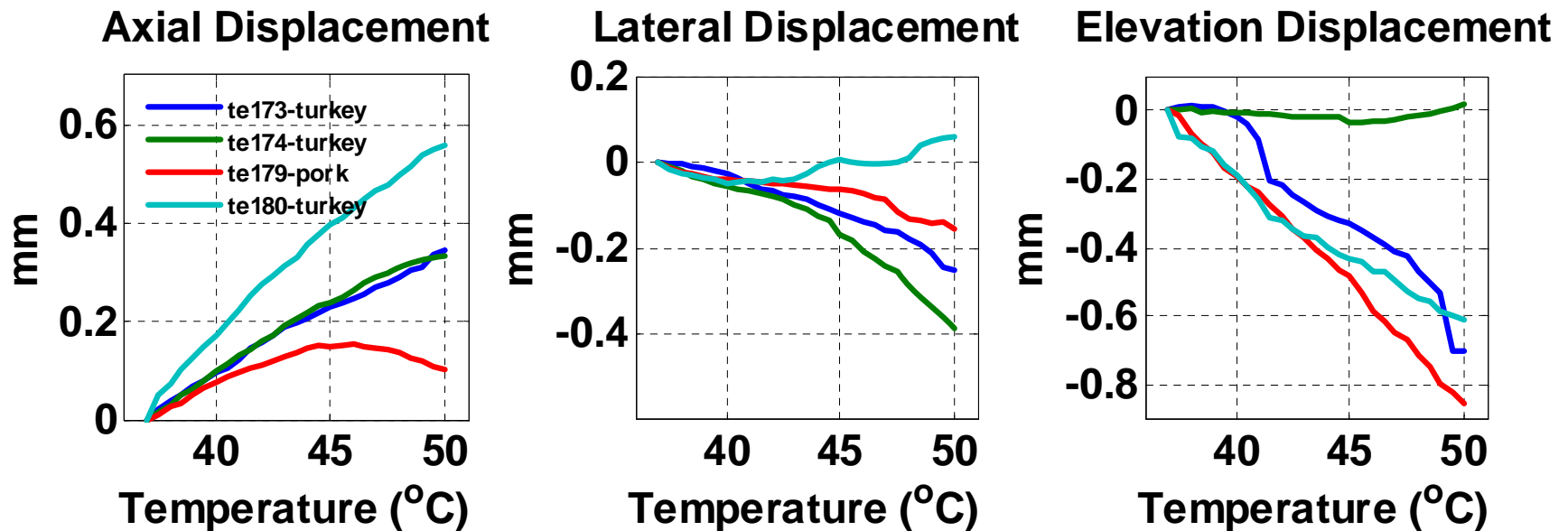
# Non-Rigid Motion in 3D



- Arrow lengths are 5X actual motion field
- Estimated using conventional optimization
- Comparable to motion seen previously in 2D



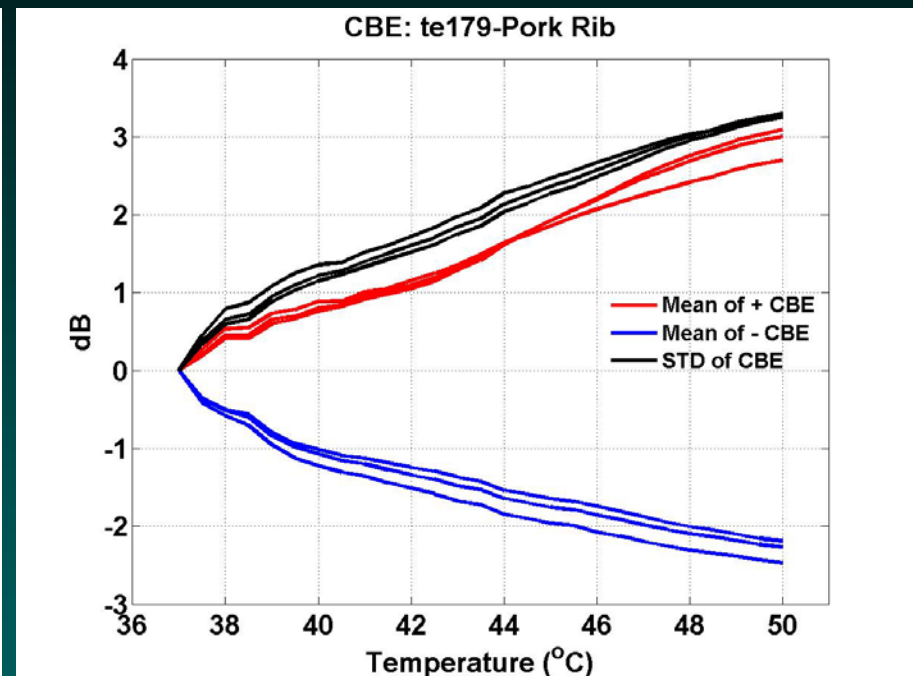
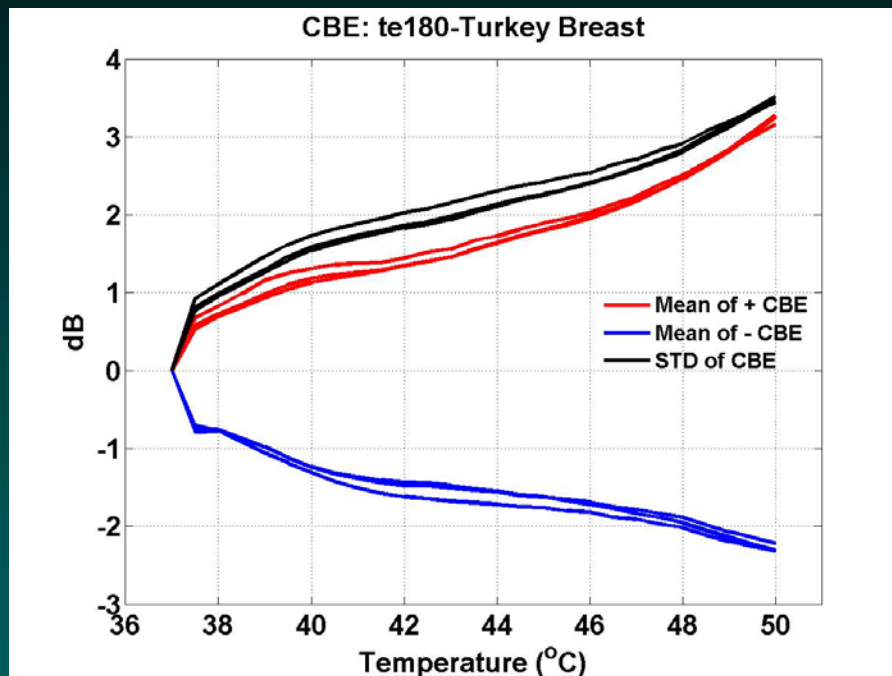
# 3D Motion with Temperature



Average Displacements in a 3 cm<sup>3</sup> Volume  
for each Tissue Specimen



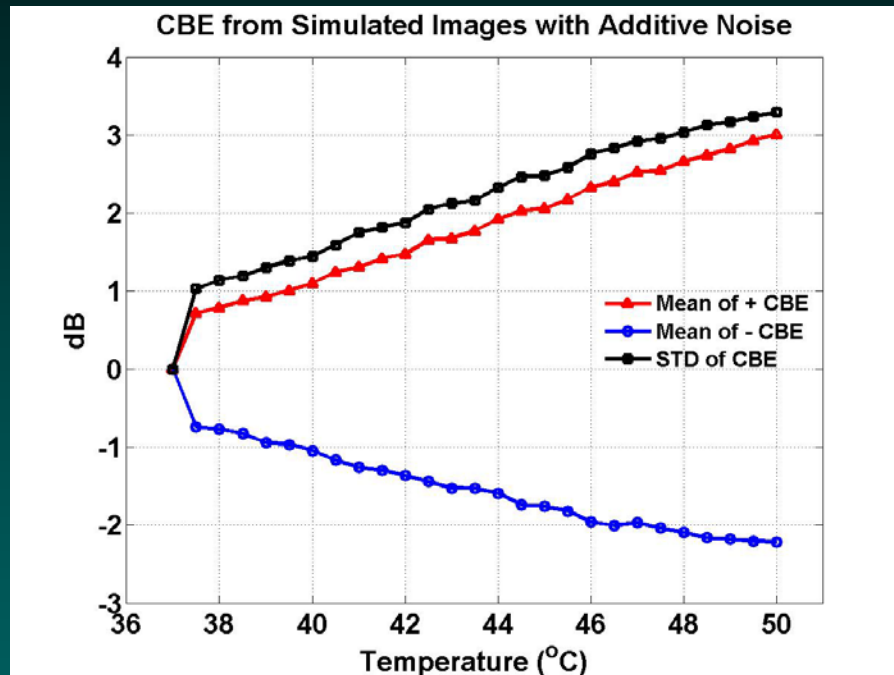
# Change in Backscattered Energy



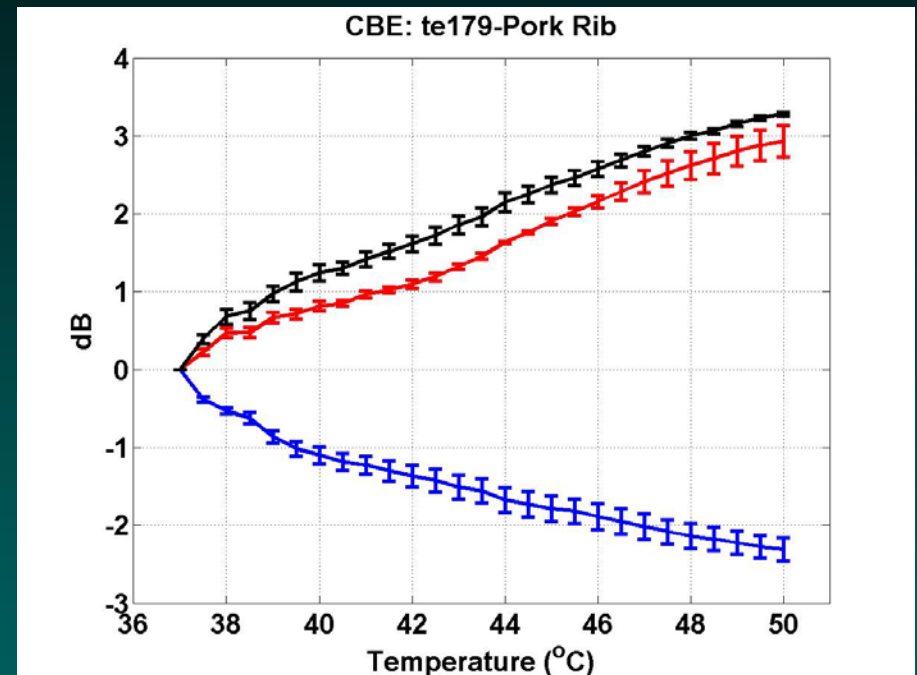
CBE Measures in Separate 1 cm<sup>3</sup> Volumes



# Change in Backscattered Energy



Simulated with Noise  
(SNR=19dB)



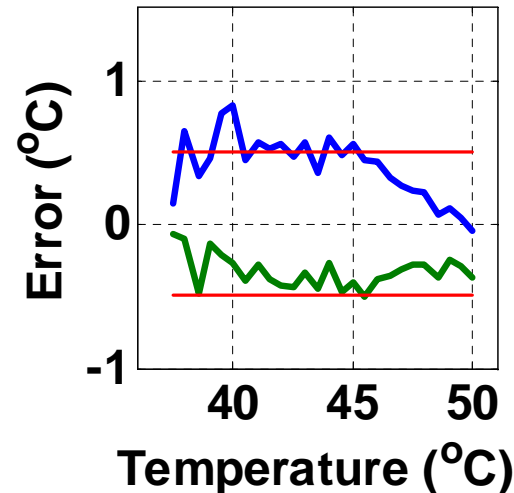
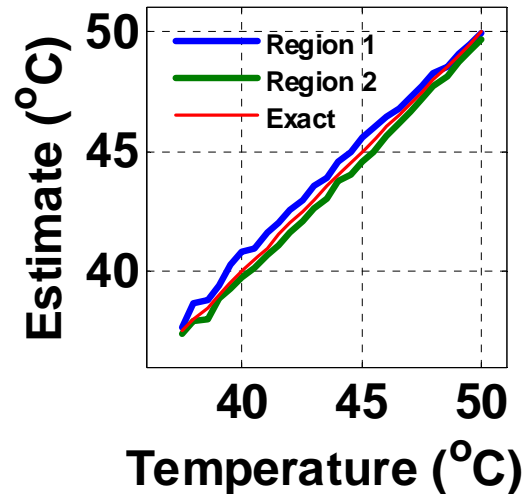
Measured in 3D



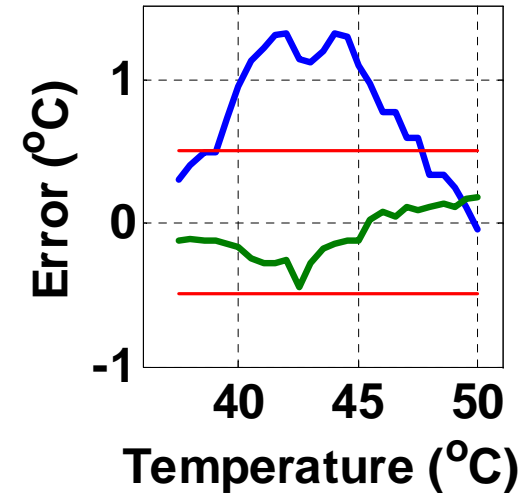
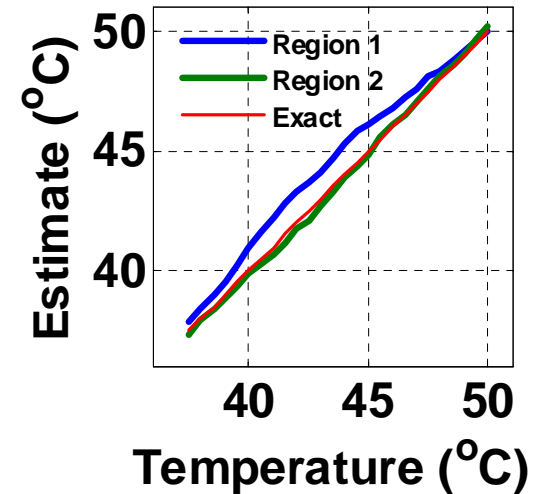
# Temperature Estimation in 3D

Estimation in two regions of  $1 \text{ cm}^3$  each, based on calibration from a third  $\text{cm}^3$  in the same tissue specimen

te179-Pork



te180-Turkey





# Summary & Conclusions

- Change in backscattered energy (CBE) was nearly monotonic & consistent in magnitude in
  - Predictions
    - Single-scatterer model
    - Multiple-scatterer simulations
  - Measured values
    - 1D isolated sites *in vitro* in liver, turkey & pork
    - 2D motion-compensated images in *in vitro* beef liver, turkey breast & pork muscle specimens
    - 2D compensated images *in vivo* in mice
    - 3D compensated images *in vitro* in turkey and pork
- We expect CBE to enable noninvasive temperature imaging for hyperthermia



# Future Directions for Thermometry Based on Ultrasonic CBE

- Refinement of the CBE model
  - ✦ Histological study of scatterer distribution
  - ✦ Evaluation of images & CBE using simulation
- Development of clinically relevant heating and measurement systems
  - ✦ Small Animal Heating with Ultrasound
  - ✦ CBE imaging with Sonotherm heating system in humans

