

Change in Ultrasonic Backscattered Energy for Temperature Imaging:

- I. Simulation with Multiple Scatterers
- II. Measurements from *In Vivo* Images

R. Martin Arthur¹, Jason W. Trobaugh¹,
William L. Straube², Jesse Parry², Yuzheng
Guo¹, and Eduardo G. Moros³

¹Electrical & Systems Engineering

²Radiation Oncology

Washington University in St. Louis.

St. Louis, MO, 63130, USA

³Radiation Oncology, University of Arkansas

Supported by NIH Grants R21 CA90531, R01 CA107558 and the
Wilkinson Trust at Washington University



Washington University in St. Louis

31st UI&TC

Arlington, VA 5/24/06

Objective of Ultrasonic Thermometry

To develop a method to produce 3D temperature maps in soft tissue during hyperthermia cancer treatment

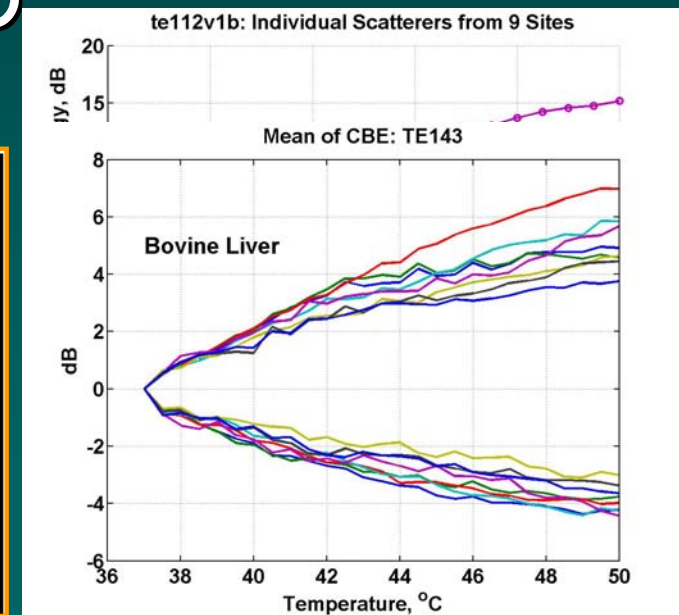
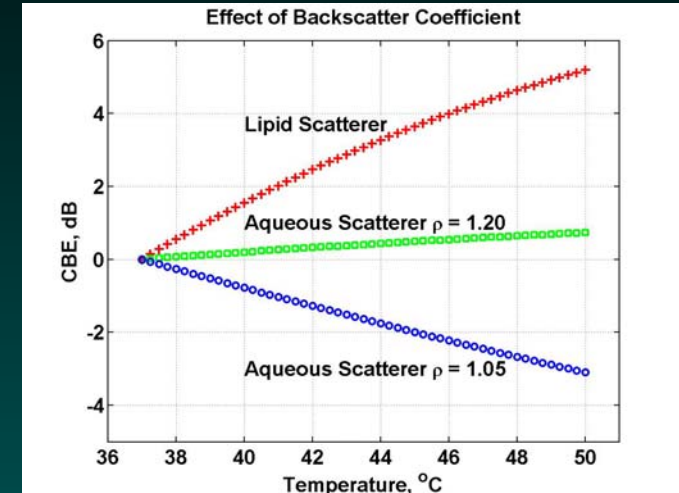
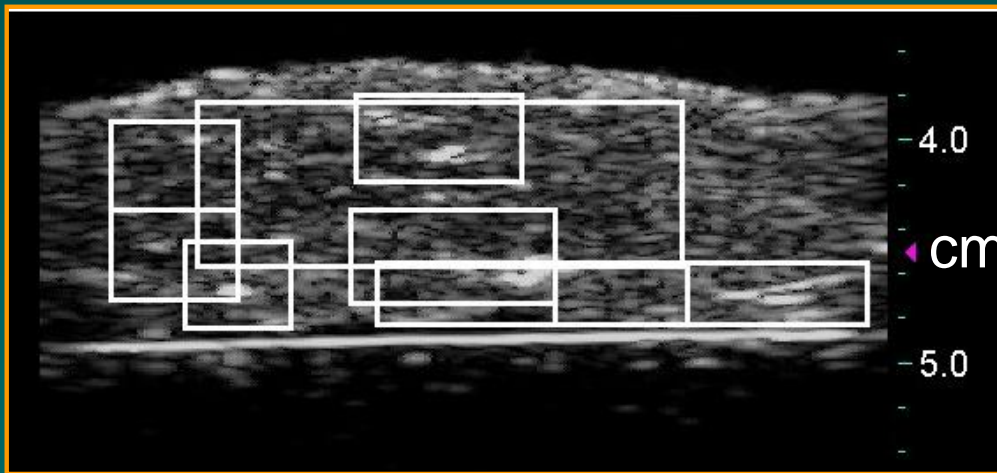
- non-invasively, conveniently at low cost with a single view from standard equipment
- with at least 0.5°C accuracy & 1 cm^3 resolution



Change in backscattered energy (CBE) as a monotonic temperature-dependent parameter

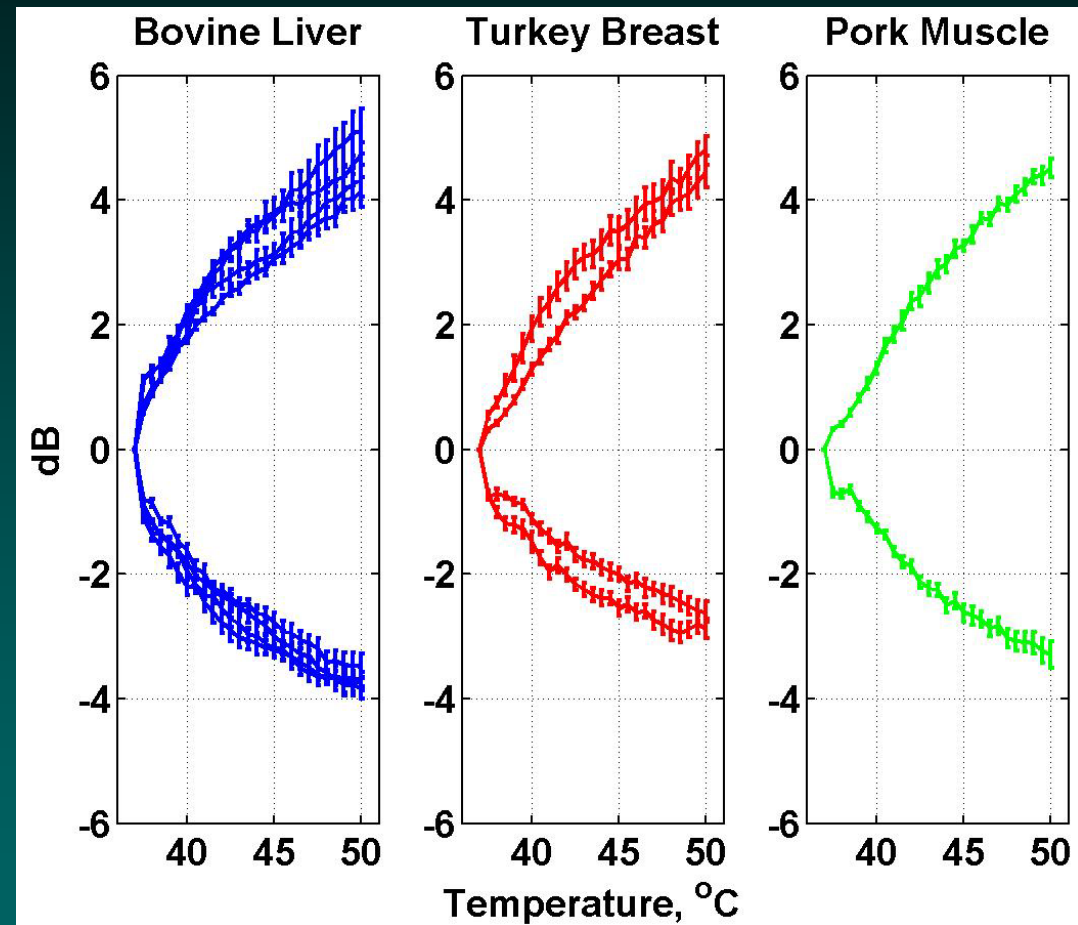
- CBE single-scatterer prediction
U Med & Bio, 20:915-922, 1994
- CBE from isolated echoes in 1D
Medical Physics, 30:1021-1029, 2003
- CBE over selected regions in 2D
IEEE UFFC, 52:1644-1652, 2005

Bovine
Liver



Change in backscattered energy (CBE) as a monotonic temperature-dependent parameter

- CBE in selected regions in 2D in 4 liver, 2 turkey & 1 pork samples
- Null tests
 - No heating ($\leq \pm 0.2$ dB)
 - Heating effects on the transducer ($\leq \pm 0.1$ dB)
 - Positioning ($\leq \pm 0.05$ dB)
- CBE in simulations of scatterer collections



I. Simulation of Scatterer Collections

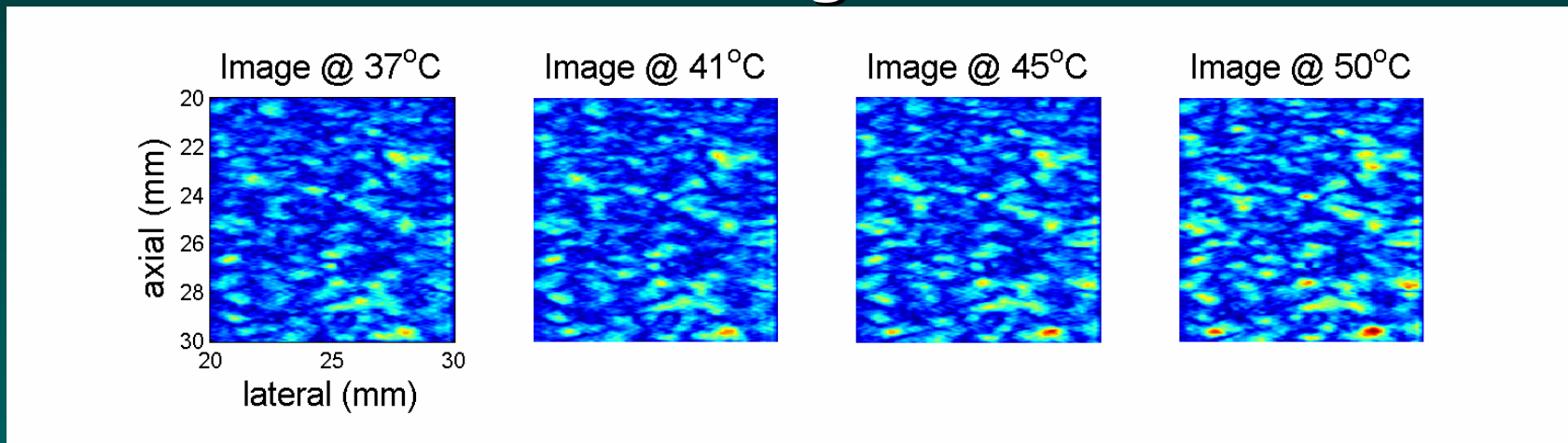
- To provide a theoretical representation for images of multiple scatterers to extend our single-scatterer model
- To study effects of noise
- To establish calibration procedures
- To determine limits on spatial resolution and temperature accuracy



Simulation Methods

Discrete-Scatterer Model

- Superposition of point-spread-functions
- Temperature dependence of individual scatterers from single-scatterer model

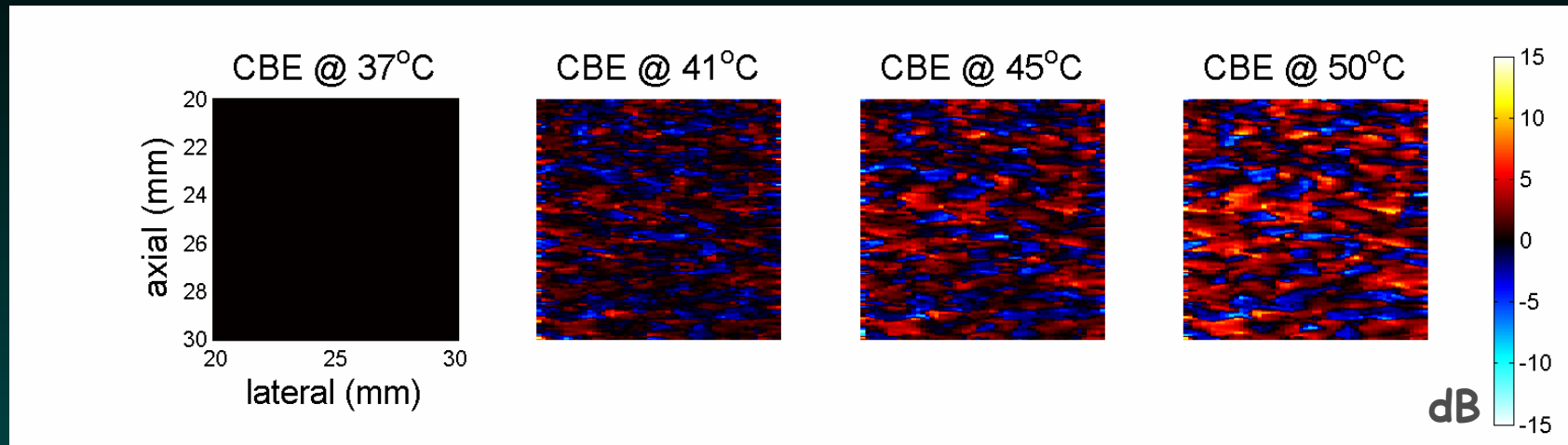


Simulated images for heating of 500 lipid and 1000 aqueous temperature-dependent scatterers randomly placed in a liver-like medium

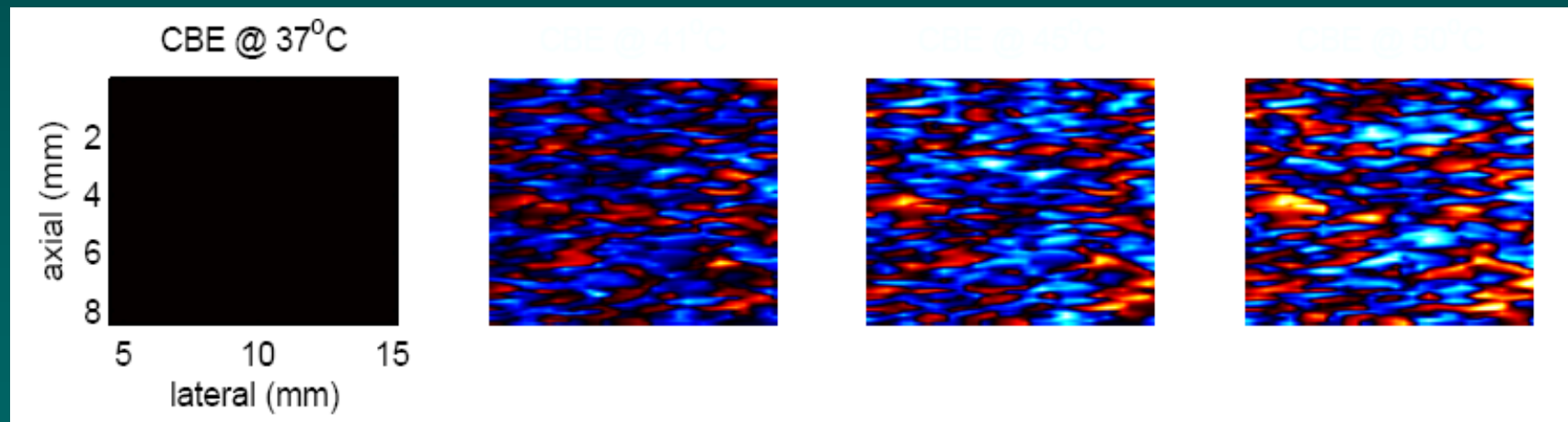
Trobaugh & Arthur, *IEEE Trans. UFFC*, 48:1594-1605, 2001



Simulated and Measured CBE



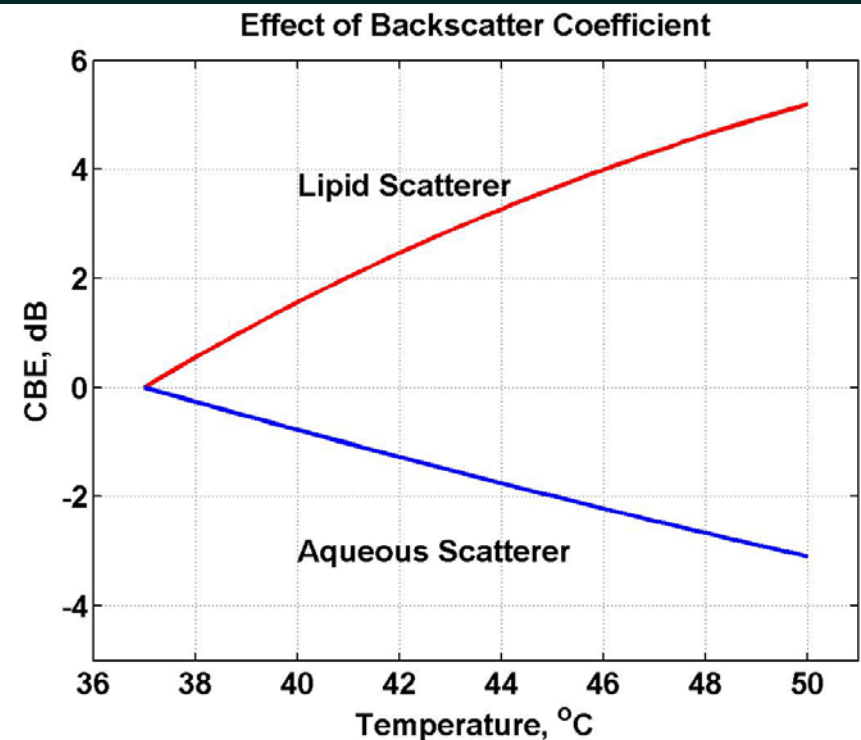
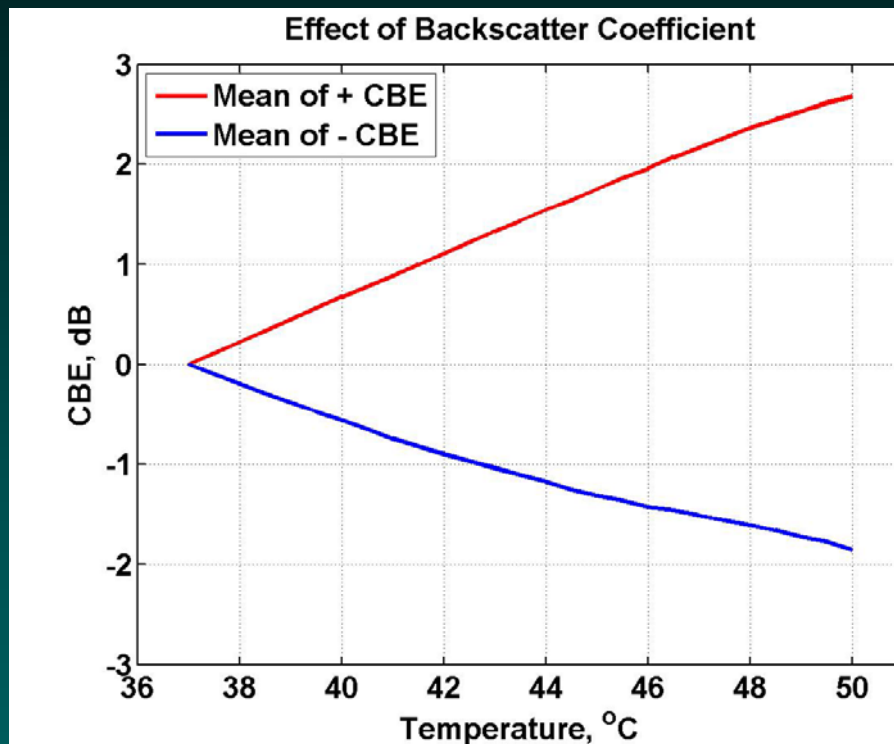
CBE from simulated images computed in the same manner used for actual images
Increase in BE (red) Decrease in BE (blue)



CBE measured in bovine liver



Single vs Multiple Scatterers

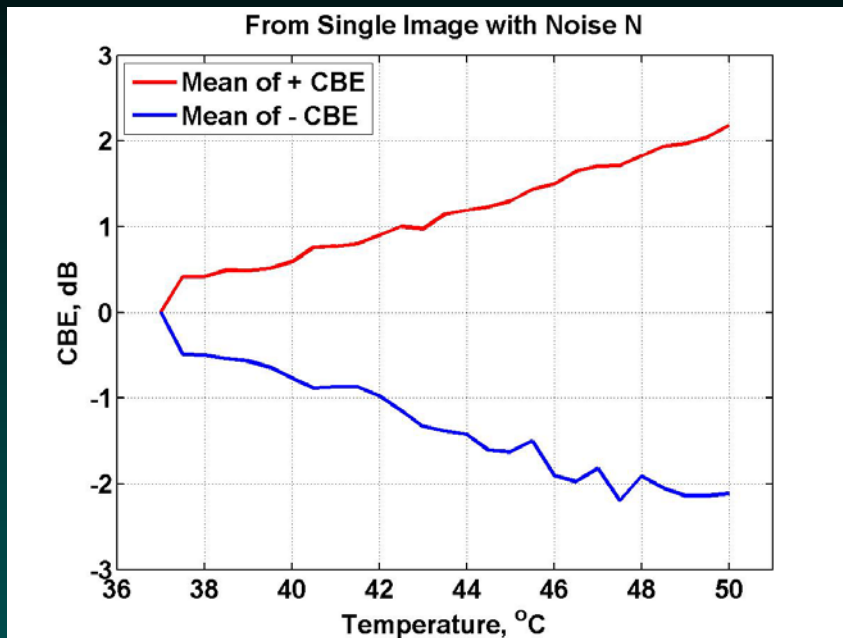


Numerical Simulation
Multiple sub-wavelength
scatterers
(500 lipid, 1000 aqueous)

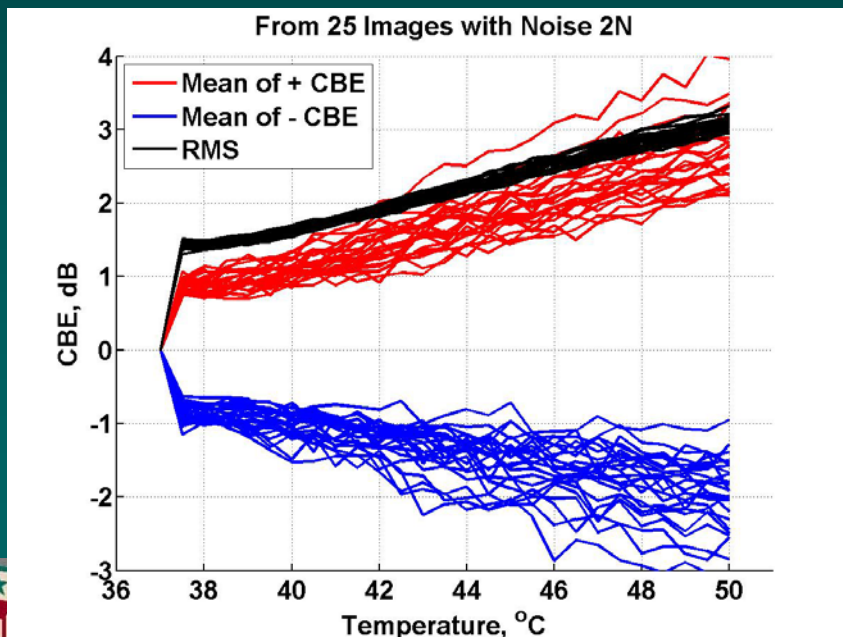
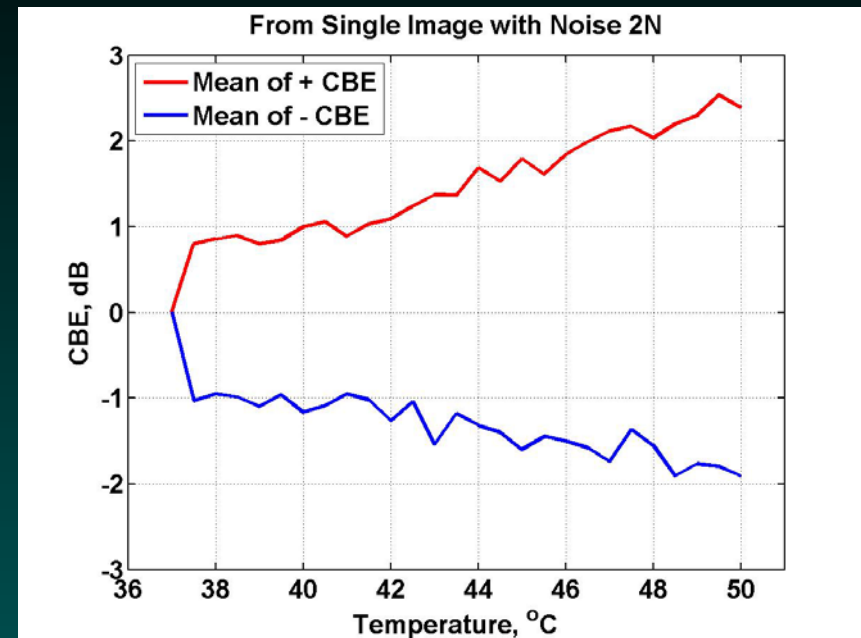
Analytic Prediction
Single sub-wavelength
scatterers



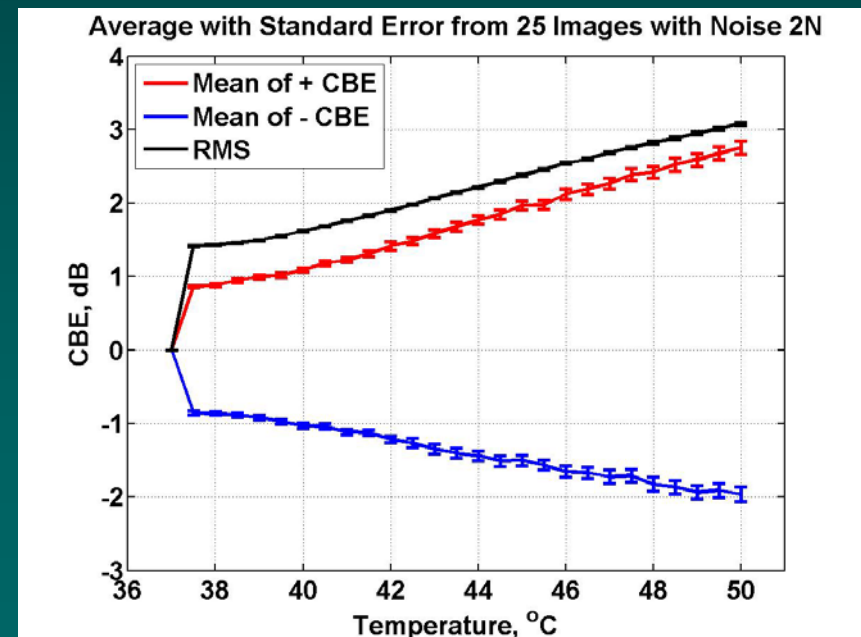
Effect of Noise in Simulated Images



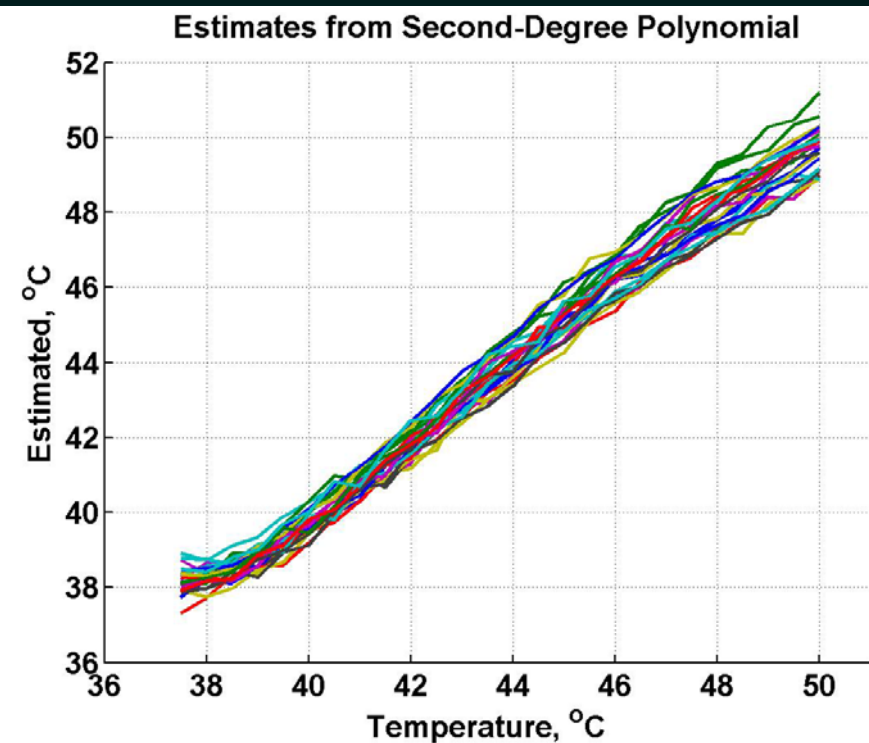
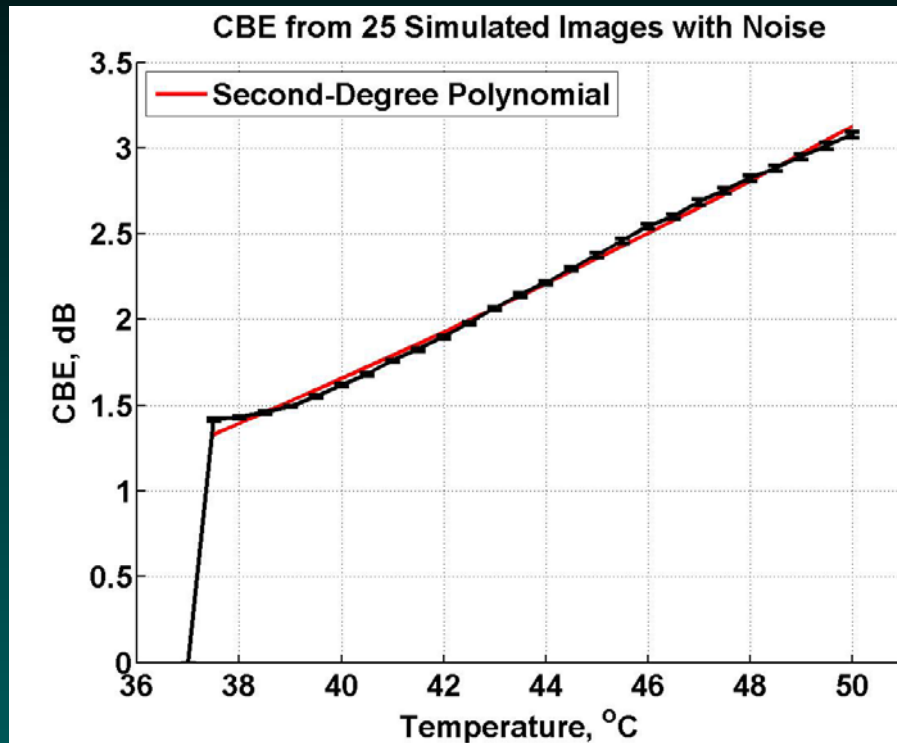
1
Image
with
Noise
Level
N



25
Images
with
Noise
Level
2N



Calibration & Estimation

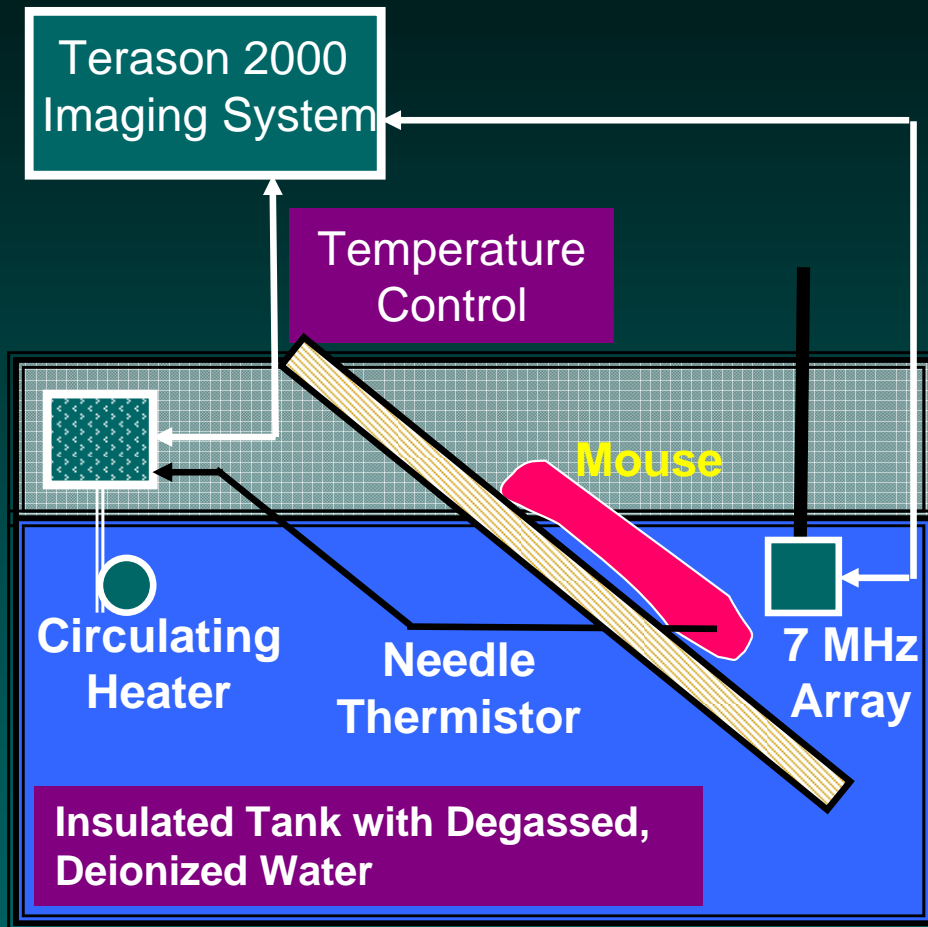


Calibration Curve
Second-degree Polynomial Fit
to CBE from Simulated
Images with Noise

Temperature Estimation
Calibration from
• Images with 1500
scatterers with
• Noise over a
• 0.3 cm^3 tissue volume



II. CBE *In Vivo*



In vivo Experimental Configuration

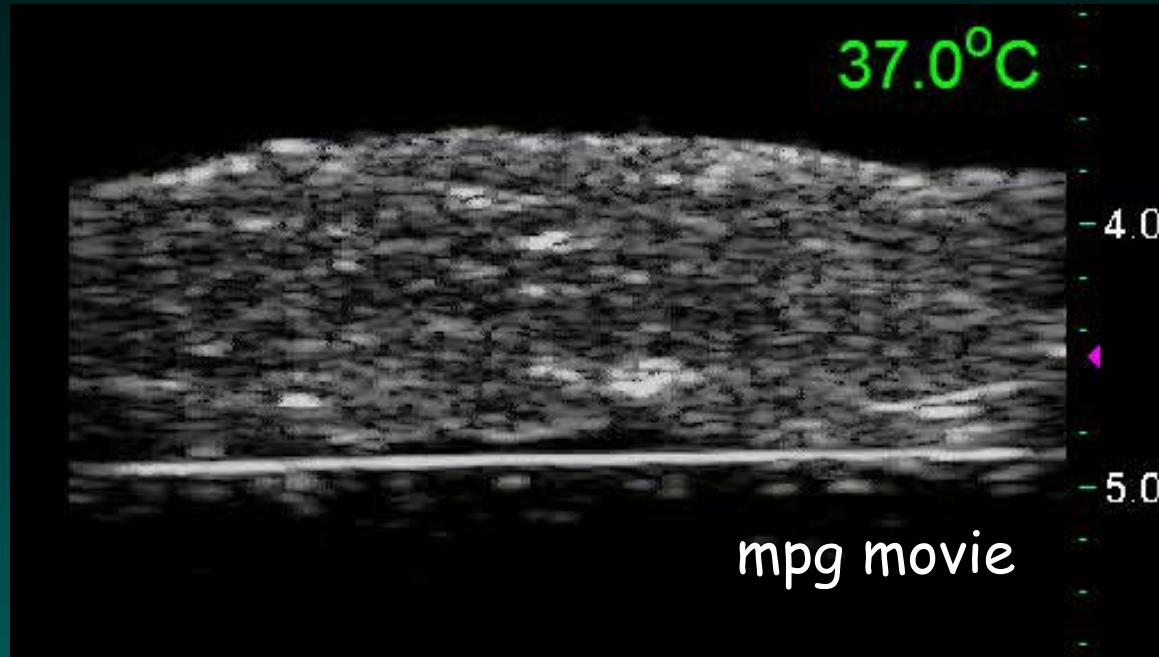


Terason 2000 (Teratech, Corp., Burlington, MA)

- 128 Element 7 MHz Linear Array
- Control of temperature from 37 to 45°C and image acquisition with AutoIt®
- Access to RF signals



Measurement of Backscattered Images



In Vitro Ultrasonic
Image of Bovine Liver

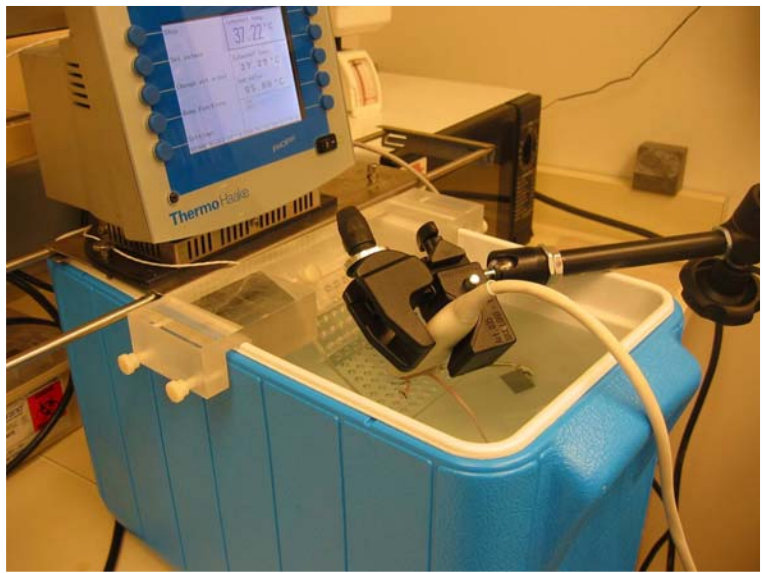
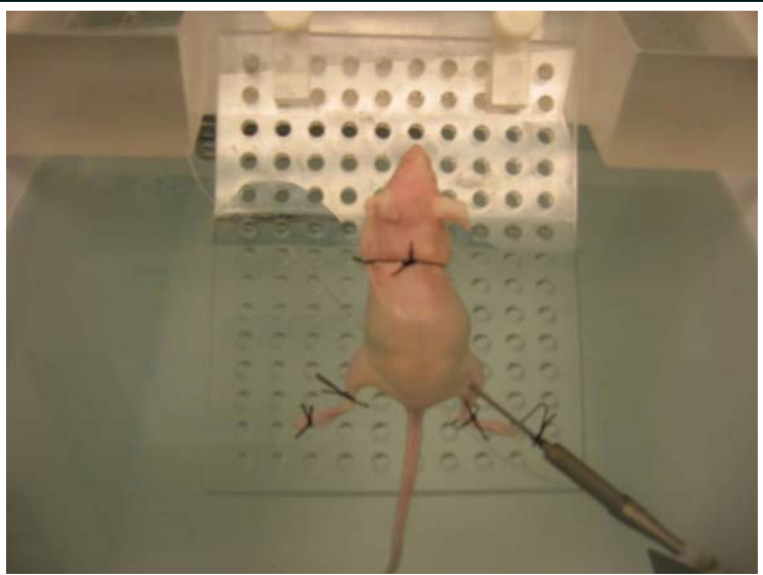
Motion was
compensated over
multiple subregions

Added Problems for
in vivo application of
CBE temperature
estimation include

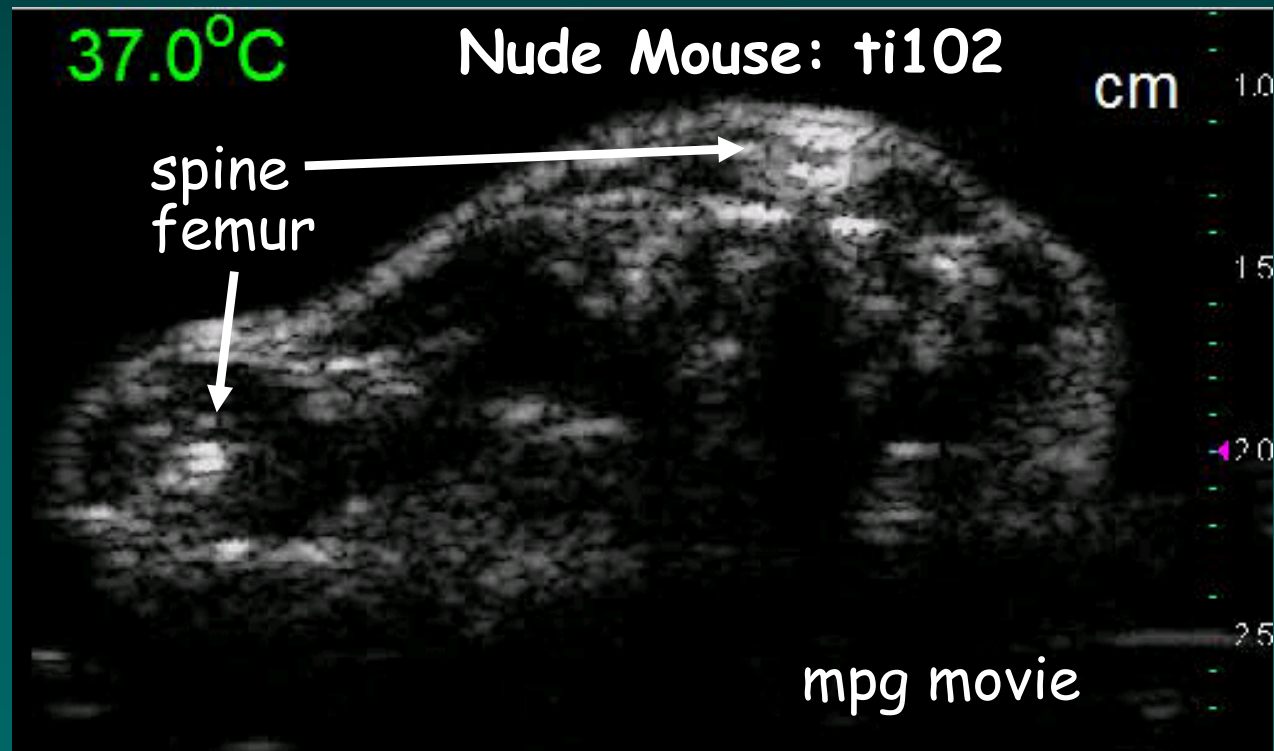
- CBE in living tissue
- Perfusion effects
- Added motion



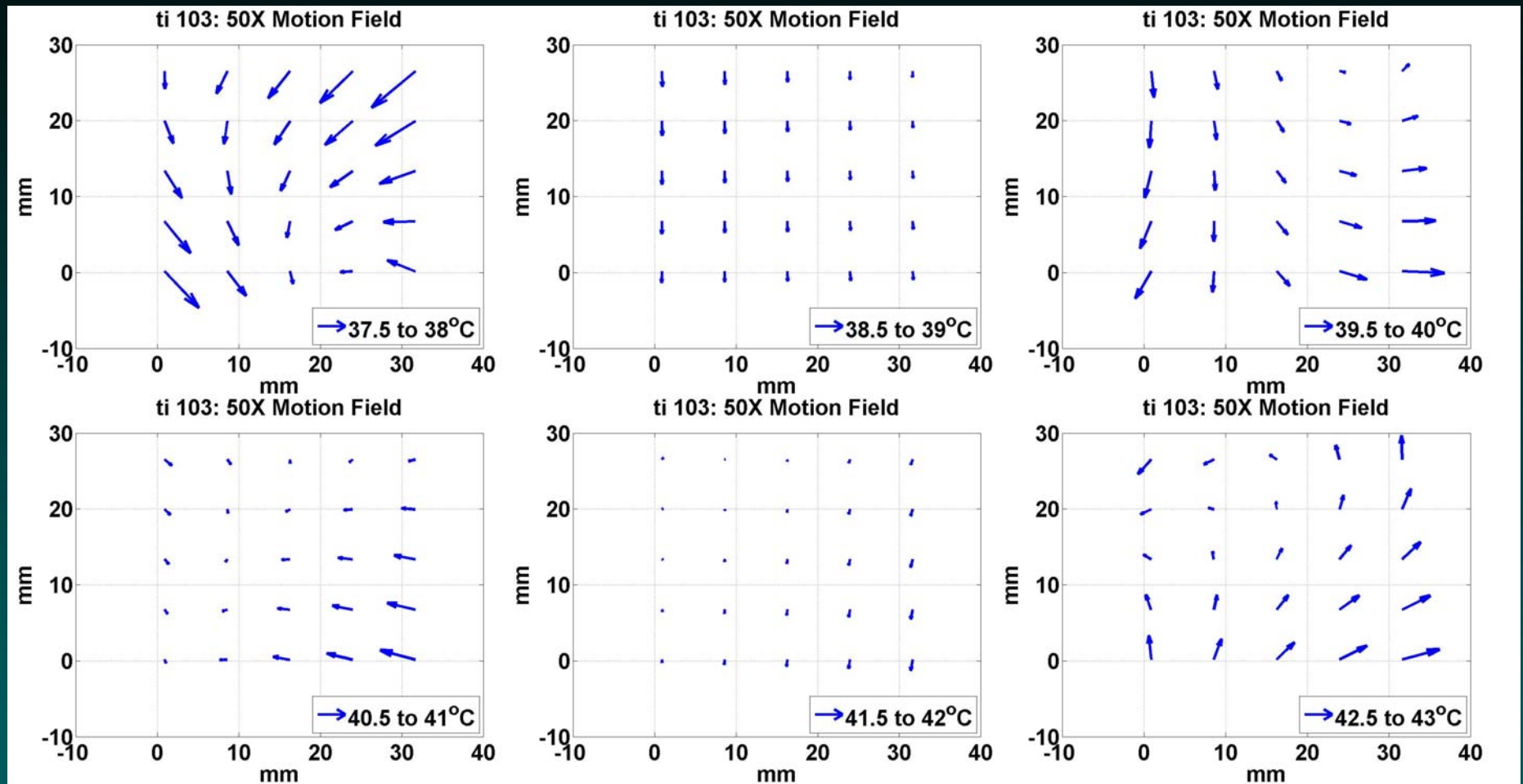
In Vivo Studies



- Performed on nude mice
 - ✦ attached to submerged angled tray
 - ✦ bilaterally implanted HT29 tumors
 - ✦ RTD thermistor in contralateral tumor
- *In vitro* procedure followed
 - ✦ from 37.0 to 45.0°C in 0.5°C steps
 - ✦ for an experiment of 0.5 hours
- Mice euthanized without recovery
- Images analyzed in a manner similar to that for *in vitro* experiments



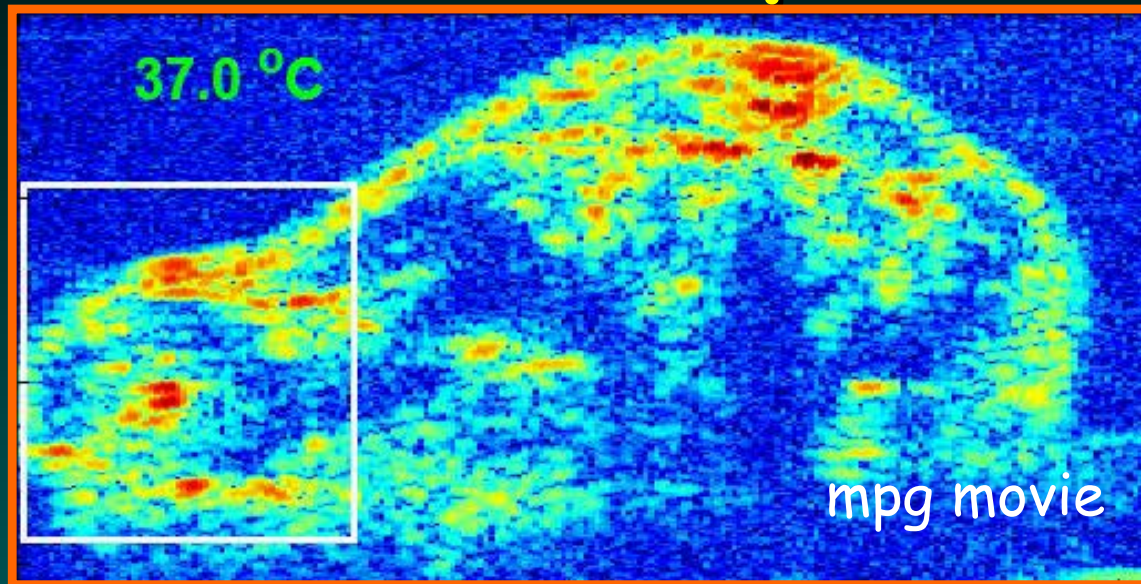
Non-Rigid Motion



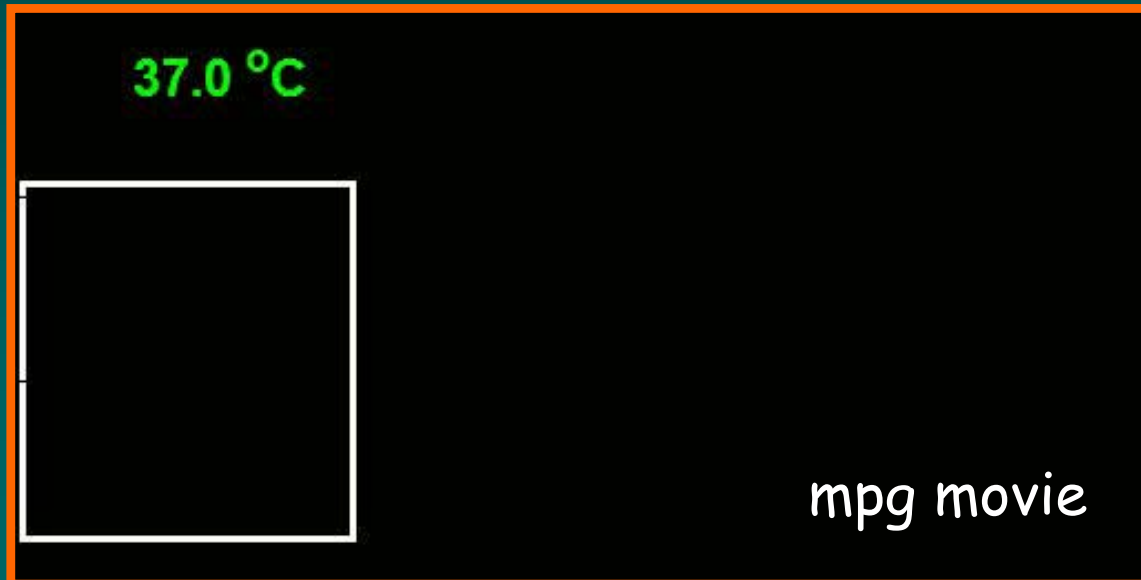
- Arrow lengths are 50 X actual motion field
- Represented as interpolation over image
- Estimated using conventional optimization



Change in Backscattered Energy in Motion-Compensated Images



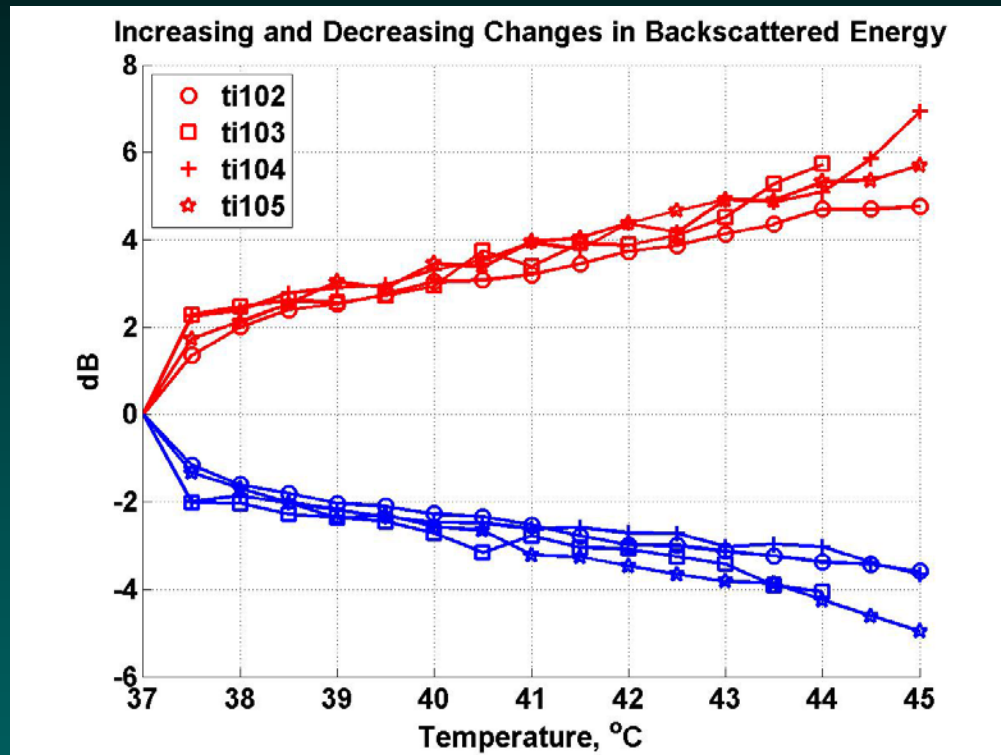
Images after
Non-Rigid Motion
Compensation



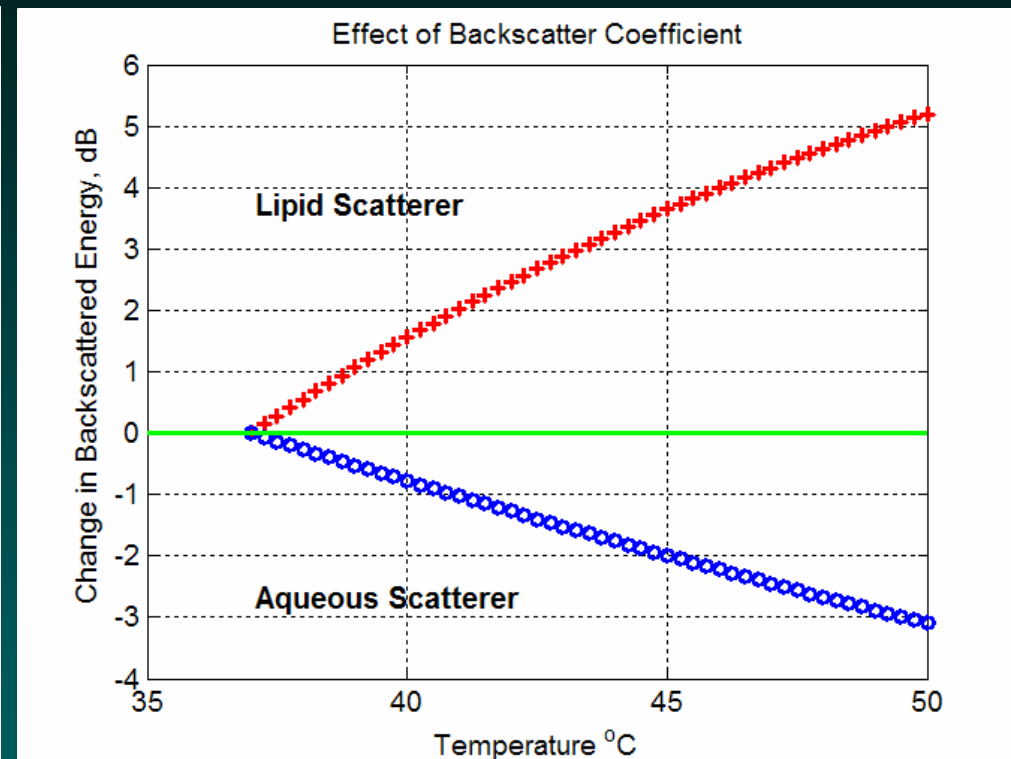
CBE
Increasing - Red
Decreasing - Blue



CBE with Temperature *In Vivo*



Measured CBE in mice

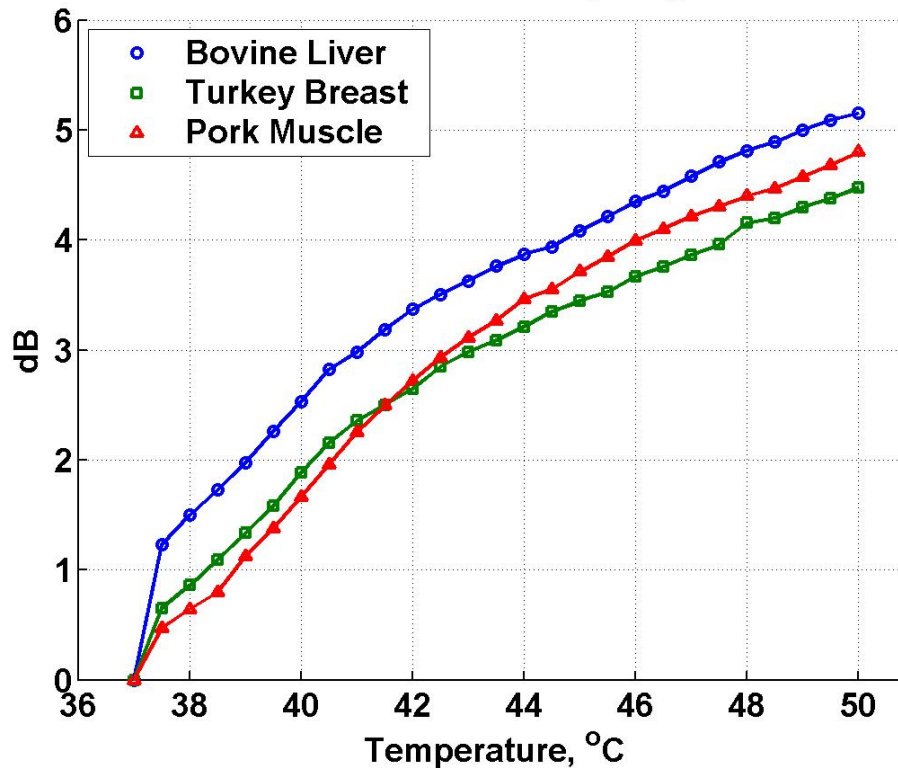


Predicted CBE in sub-wavelength scatterers



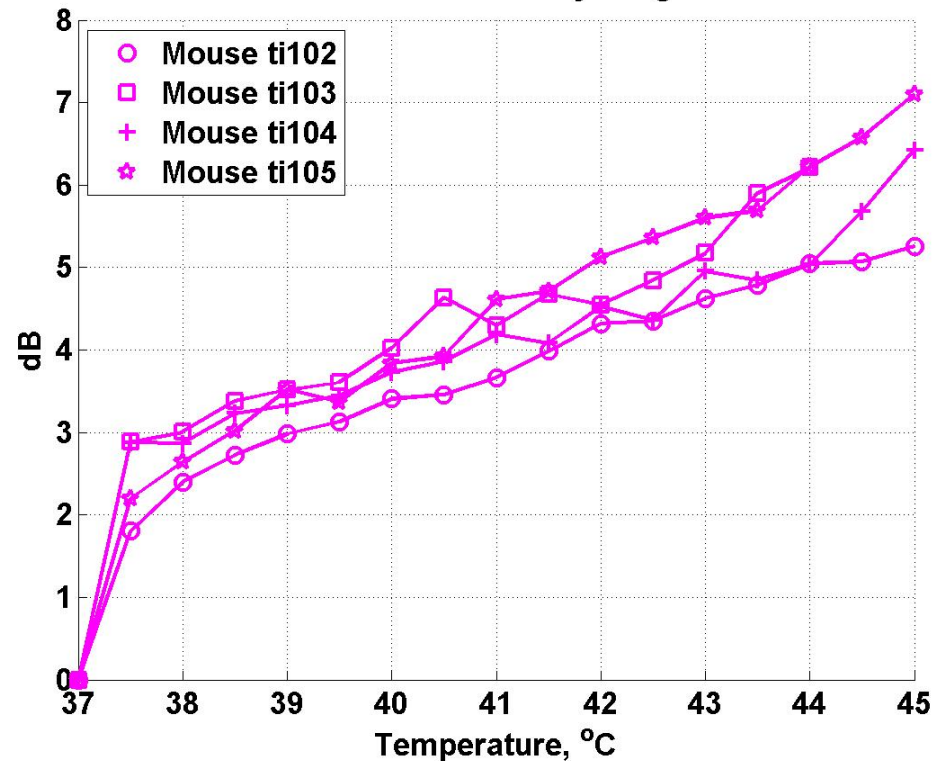
CBE with Temperature

CBE in Phased-Array Images



In Vitro

CBE in Phased Array Images



In Vivo

- CBE is nearly monotonic with temperature
- Calibration of CBE may enable temperature imaging



Summary & Conclusions

- Change in backscattered energy (CBE) was nearly monotonic and consistent in magnitude in
 - Predictions
 - Single-scatterer model
 - Multiple-scatterer simulations
 - Measured values
 - 1D isolated sites in *in vitro* beef liver, turkey breast & pork muscle specimens
 - 2D motion-compensated images in *in vitro* beef liver, turkey breast & pork muscle specimens
 - 2D motion-compensated images *in vivo* in mice
- We expect CBE to enable noninvasive temperature imaging for hyperthermia



Future Directions for Thermometry Based on Ultrasonic CBE

- Refinement of the CBE model
 - ✦ Histological study of scatterer distribution
 - ✦ Evaluation of images & CBE using simulation
- Estimation of temperature from simulations and measurements
- Development of clinically relevant heating and measurement systems
 - ✦ Small Animal Heating with Ultrasound
 - ✦ Scanning Ultrasound Reflector Linear Array

