# A Novel Spike Distance

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# A novel spike distance

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Department of Biology, MS 008 Brandeis University, Waltham MA e-mail: vrossum@swallow.bio.brandeis.edu effective but it misses all temporal structure in the spike trains.

## **Abstract**

The discrimination between two spike trains is a fundamental problem, both for the experimentalist and for the nervous system itself. We introduce a measure for the distance between two spike trains. The distance has a time constant as a parameter. Depending on this parameter, the distance interpolates between a coincidence detector and a rate difference counter. The dependence of the distance on noise is studied with an integrate and fire model. For an intermediate range of the time constants, the distance depends linearly on the noise. This property can be used to determine the intrinsic noise of a neuron. *To appear in Neural Computation*.

# 1 Introduction

In the analysis of experimental neural data one often encounters the question "How similar are these two spike trains?". For instance, if one studies the effect of a certain manipulation, or if one studies how reproducible the neuron's response is. A problem is that it is not really known what information to look for in the spike train. In particular cases the precise timing is known to be important, whereas in other cases only the number of spikes in a certain interval seems of importance (Rieke, Warland, de Ruyter van Steveninck and Bialek 1996). The nervous system itself is possibly confronted with the same question of similarity. For instance when it has to respond to a certain visual cue and has to decide what the appropriate response is ("Was that really a tiger?!").

One approach to address this question is to introduce a distance which measures the (dis)similarity of two spike trains. If the distance between two spike trains is small enough, one can assume that the inputs were identical. Alternatively, distance measures can be used in a forced choice experiment in which the spike train is compared to different templates. In that case the template with the smallest distance to the trail should be chosen. Previously introduced measures to compare spike trains are, among others,

1) The total spike count. Measure the total number of spikes in the spike trains and compare the counts. This method is quite

2) To resolve temporal structures, the spikes can be binned and the number of spikes per bin is counted. Next, one measures the number of coincident spikes (see e.g. Kistler, Gerstner and van Hemmen 1997). Alternatively, the count is interpreted as a vector in N-dimensional space, where N is the number of bins. The distance to other spike trains can be calculated using a N-dimensional Euclidean distance (Geisler, Albrecht, Salvi and Saunders 1991, MacLeod, Backer and Laurent 1998). A disadvantage of the binning procedure is that it does not distinguish between a spike shifted so that it just drops out of the bin, and a spike shifted many bin durations. And a spike which is shifted but stays within the bin, is treated as a spike which was not shifted at all. These might not always be desired effects if the spike timing matters.

3) A more flexible distance measure is needed which takes the temporal structure into account, but avoids the problems associated with binning. In a set of comprehensive papers Victor and Purpura introduced a measure based on a cost function (Victor and Purpura 1996, Victor and Purpura 1997). Two processes differentiate one spike train from another: First, spikes can be deleted or inserted. Secondly, spikes can be shifted in time. Victor and Purpura attributed to both processes a certain (arbitrary) cost and calculated how much it would cost to transform one spike train into the other one. The cost of insertion/deletion was fixed to one. If no cost was associated with the shifting process, the total cost was just the difference in the total number of spikes. Otherwise, the cost function for the shift was taken to be a monotonic increasing function of the spike time difference. Although this method has been applied successfully (MacLeod et al. 1998), the calculation of the full cost function is quite involved. The reason is that it is not always clear where a displaced spike came from, and if the number of spikes in the trains is unequal, it can be difficult to determine which spike was inserted/deleted.

Here we introduce a spike distance closely related to the distance introduced by Victor and Purpura, yet it is easier to calculate and has a physiological interpretation. The distance is used to measure the intrinsic noise of a model neuron.

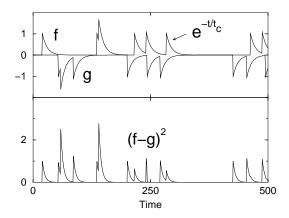


Figure 1: The definition of the distance. Upper graph: Two spike trains (one flipped) are convolved with an exponential with time constant  $t_c$ . Lower graph: The difference squared of the spike trains. The distance is given by the integral of this curve.

# 2 A novel measure

With the goal to have a simple distance measure we propose the following: Given a spike train with spike times  $t_i$ ,

$$f^{\text{orig}}(t) = \sum_{i}^{M} \delta(t - t_i), \tag{1}$$

where we will assume that all  $t_i > 0$ . Replace the delta-function associated which each spike with an exponential function, that is, add an exponential tail to all spikes,

$$f(t) = \sum_{i}^{M} H(t - t_i)e^{-(t - t_i)/t_c}.$$
 (2)

Here  $t_c$  is the time constant of the exponential function and H is the Heaviside step function  $(H(x) = 0 \text{ if } x < 0 \text{ and } H(x) = 1 \text{ if } x \ge 0)$ . In principle, one could convolve with functions other than the exponential. Our choice for the exponential function was motivated by its causality, its simplicity, and its possible biological interpretation (see Discussion). The distance between two trains f and g we define as, Fig. 1,

$$D^{2}(f,g)_{t_{c}} = \frac{1}{t_{c}} \int_{0}^{\infty} \left[ f(t) - g(t) \right]^{2} dt.$$
 (3)

The distance is the Euclidean distance of the two filtered spike trains with  $t_c$  as a free parameter.

To get a feel for the distance, consider the two limits of  $t_c$ . For  $t_c$  much smaller than the inter-spike interval, the smeared functions f and g contribute to the integral only if the spikes are not more than  $t_c$  apart. This is very similar to a coincidence detection. For most spike trains coincident spikes can be neglected in the limit of zero  $t_c$ , thus if f contains M and g contains N spikes one has

$$\lim_{t_c \to 0} D^2(f, g)_{t_c} = \frac{1}{t_c} \int_0^\infty \left[ f^2(t) + g^2(t) \right] dt = \frac{M + N}{2}. \tag{4}$$

The distance counts the non-coincident spikes.

In the opposite limit, for large  $t_c$ , the main contribution to the integral comes from times when the last spike has passed but the exponent has still not decayed. Assuming that f(g) contains M(N) spikes, one can approximate

$$\lim_{t_c \to \infty} D^2(f, g)_{t_c} = \frac{1}{t_c} \int_0^\infty (M e^{-t/t_c} - N e^{-t/t_c})^2 dt = \frac{(M - N)^2}{2}.$$
 (5)

In this limit D measures the difference in total spike count. Note that it is important that the upper limit of the integral is taken to be infinity (or, in practice until the tail of the last spike died out), instead of the time of the last spike.

The distance thus interpolates between the two extremes of coincidence detection and measuring difference in total spike count. The distance measure is very easy to implement numerically (for the best results the integral between spikes and after the last spike can be done analytically, after filtering the spike trains this leaves a sum of N+M terms).

Changing integration variables leads to an alternative expression for the distance

$$D^{2}(f,g) = \frac{1}{2} \int_{-\infty}^{\infty} C_{f-g,f-g}(t) e^{-|t|/t_{c}} dt,$$
 (6)

where  $C_{f-g,f-g}(t)$  is the autocorrelation of difference of the raw spike trains,  $f^{\text{orig}}(t) - g^{\text{orig}}(t)$ . This shows that the distance can be interpreted as the weighted integral over the autocorrelation, with the weighting depending on  $t_c$ . It also shows that the distance is invariant under time reversal, that is, the distance is the same if the exponential tails were attached to the other sides of the spikes.

# 2.1 Analytical results

For some simple cases we can derive analytical results. Let us consider the distance between two almost identical spike trains. First consider the insertion of a single spike at time  $t_i$  into train f, other than that the spike trains are identical, that is,

$$g(t) = f(t) + H(t - t_i)e^{-(t - t_i)/t_c}$$

The distance is

$$D_{\text{insertion}}^{2}(f,g) = \frac{1}{t_{c}} \int_{t_{c}}^{\infty} e^{-2(t-t_{i})/t_{c}} = \frac{1}{2}.$$
 (7)

The removal of a spike yields the same answer. Note that the result is independent of  $t_c$ .

Now suppose a spike is shifted from  $t_i$  in spike train f to time  $t_i + \delta t$  in g

$$g(t) = f(t) - H(t - t_i)e^{-(t - t_i)/t_c} + H(t - t_i - \delta t)e^{-(t - t_i - \delta t)/t_c}$$

which yields a distance,

$$D_{\text{displace}}^{2}(f,g) = \frac{1}{t_{c}} \int_{t_{i}}^{t_{i}+\delta t} e^{-2(t-t_{i})/t_{c}} + \frac{1}{t_{c}} \int_{t_{i}+\delta t}^{\infty} [e^{-(t-t_{i})/t_{c})} - e^{-(t-t_{i}-\delta t)/t_{c}}]^{2}$$

$$= 1 - e^{-|\delta t|/t_{c}}. \tag{8}$$

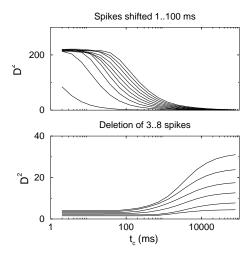


Figure 2: The effect of the deletion and shifting of spikes on the distance versus  $t_c$ . Upper graph: All the spikes in the second spike train are shifted 1..100 ms with respect to the first train. At large  $t_c$  this shift does not contribute to the distance. The spike trains were Poisson trains with a duration of 10 s and a rate of 20 Hz. Lower graph: At random positions 3..8 spikes are deleted from the second spike train (lower to upper curve). The distance is largest at large  $t_c$ .

Which is unity for small  $t_c$  and vanishes for large  $t_c$ . The ratio of distances due to spike insertion and due to displacement depends on  $t_c$ . For a shift  $\delta t = t_c \ln(2)$ , insertion and displacing cost the same. Note, however, that displacing a spike never costs more than insertion/removal of two spikes. The reason is that shifting a spike can always be done by removing the spike at time t and re-inserting it at time  $t + \delta t$ .

### 2.2 Correlation effects

When one considers two trains in which more spikes are changed, the distance is more complicated and certainly not always equal to the sum of the individual displacement and insertion distances. As an example consider the case where two spikes, a time T apart, are both displaced a time  $\delta t$ ; no other spike occurs between the two. For this case one finds

$$D^{2}(f,g) = 2 \left[ 1 - e^{-|\delta t|/t_{c}} \right] - 2e^{-|T|/t_{c}} \left[ \cosh(\delta t/t_{c}) - 1 \right], \quad (9)$$

In Fig. 2 the distance is plotted for various amounts of shift. The first term is twice the single spike displacement distance, Eq. (8). The second term is due to the correlation and is always negative: thus the total distance of displacing two spikes is less if the spikes are close. This seems a natural phenomena as the spike trains will look more similar when two neighboring spikes are shifted than when two spikes far apart are shifted. However, proper description of such effects calls for a more complex distance measure with the introduction of extra time-scales (Victor and Purpura 1997).

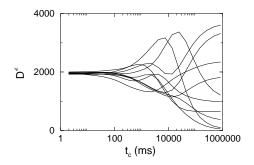


Figure 3: Distance between two independent Poisson trains. The distance is on average constant across  $t_c$ , but shows large fluctuations at large  $t_c$ .

Likewise, one can study the insertion of two spikes, time *T* apart. For that case one finds:

$$D^{2}(f,g) = \frac{2}{2} + e^{-T/t_{c}},$$
(10)

that is, the cost of insertion two spikes close together is larger than the cost of inserting two distant spikes. Equivalently, when more than one spike is inserted the distance will increase with increasing  $t_c$ , see Fig. 2.

#### 2.3 Distance between uncorrelated Poisson trains

Next, we calculate the distance between two uncorrelated Poisson spike trains both with a rate  $\rho$ . For small  $t_c$  the distance measures the number of spikes, see Eq.(4). Assuming a total duration of T, on the average  $\rho T$  spikes will be produced, so for small  $t_c$ ,  $D^2 = \rho T$ . On the other hand, for large  $t_c$ , according to Eq.(5) the distance approaches  $(M-N)^2/2$ , where M and N denote again the number of spikes in the trains. The expectation value for  $(M-N)^2$  for two Poisson processes is  $2\rho T$ , hence for large  $t_c$  one has  $D^2 = \rho T$ . The average distance is thus identical at small and large  $t_c$ . Alternatively, one can use Eq.(6) and that  $C_{f-g,f-g} = C_{f,f} + C_{g,g} - 2C_{f,g} = 2\rho T\delta(t)$ , which yields  $D^2 = \rho T$  independent of  $t_c$ .

Numerical simulations are shown in Fig. 3. The distance shows large fluctuations for large  $t_c$ ; the difference in the number of spikes fluctuates more strongly than the number of non-overlapping spikes. The reason is that the difference can be interpreted as a variance, while the number of non-overlapping spikes behaves more like a mean value; it is well known that the variance is a more variable quantity than the mean.

# 3 Distance between two noise driven spike trains

Next, we study how the distance varies in response to changes in the input for a spiking neuron. We use a leaky integrate and fire neuron with a timeconstant of 50 ms. The stimulus is a Gaussian distributed variable with zero mean and 10 ms temporal correlation.

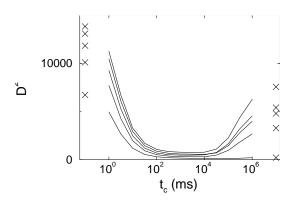


Figure 4: Distance between a spike train and the spike train with noise added to the input. The different lines correspond to different amounts of noise: standard deviation 2, 4, 6, 8, and 10% of stimulus standard deviation (lower to upper curve). The crosses indicate the limits  $t_c \to 0$  and  $t_c \to \infty$ . Note the minimum of the distance at intermediate  $t_c$ .

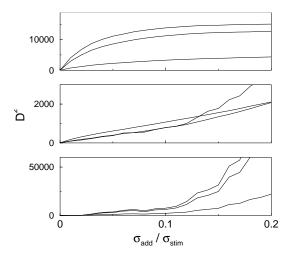


Figure 5: Same data as Fig. 4, but here the distance is plotted versus the noise added to the stimulus. For different  $t_c$  there are different power laws between the distance and the noise. The standard deviation of the noise is denoted as fraction of the stimulus standard deviation. Because of the different y-scaling the plots were split for different  $t_c$  values: upper graph,  $t_c = 0$ , 1, 10; middle graph  $t_c = 100,1000,10000$  (linear regime); lower graph  $t_c = 10^5,10^6, \infty$ .

Its variance is adjusted to give an average spike frequency of 20 Hz. To compare spike trains this stimulus is repeated across trials, and non-repeating Gaussian noise is added.

The standard deviation of the noise,  $\sigma_{add}$ , was up to 10% of the standard deviation of the stimulus. In Fig. 4 we plot the distance as  $t_c$  is varied. As expected, the distance initially drops as spike time differences due to slightly displaced spikes are smoothed out. However, for large  $t_c$  the distance increases again. This contrasts with the distance between two Poisson spike trains were the average distance was constant across  $t_c$ . For the integrate and fire neuron, noise will both shift as well as insert/delete spikes. The membrane time constant introduces temporal correlations, leading to a minimal distance when  $t_c$  is roughly of the order of the integration time constant. Why the precise value is actually larger than the membrane time constant is not clear.

The dependence of the distance on the amount of added noise varies for different values of  $t_c$ , see Fig. 5. Unfortunately, there is no obvious analytical approach to determine the distance as function of the noise for the integrate and fire model, instead we rely on simulations. We found approximately a power law relation between distance and noise, with the exponent depending on  $t_c$ . For small  $t_c$  it holds that  $D^2 \propto \sqrt{\sigma_{add}}$ , whereas for large  $t_c$  one has  $D^2 \propto \sigma_{add}^{2...4}$ . However, for a large region of intermediate  $t_c$ , roughly corresponding to the valley region in Fig. 4, one has  $D^2 \propto \sigma_{add}$ .

# 3.1 Estimating intrinsic noise

The smooth dependence of the distance on the noise can be used to measure the intrinsic noise of a neuron. To this end we assume that there is an intrinsic noise source in the neuron which is additive to the input (Tuckwell 1988, Gerstein and Mandelbrot 1964). By mixing additional non-repeating noise with the input and extrapolating the distance, the intrinsic noise can be estimated, Fig. 6. The standard deviation at the input of the spike generator is  $\sigma_{total} = \sqrt{\sigma_{add}^2 + \sigma_{intrinsic}^2}$ , therefore the distance is best considered as a function of  $\sigma_{add}^2$ . In practice, one plots  $D^4$  versus  $\sigma_{add}^2$  and fits a straight line. The intrinsic noise is reconstructed from the intercept of the line with the x-axis, see Fig. 6B.

This method is borrowed from electrical engineering and psychophysical studies. There one measures, for instance, the detection threshold of a visual stimulus as noise is added to the stimulus (Pelli 1990, Lu and Dosher 1999). This detection threshold is commonly proportional to the signal to noise ratio of the stimulus, which then allows determination of the intrinsic noise.

To test the approach we simulate an integrate and fire neuron with an intrinsic noise source and tried to estimate the amount of intrinsic noise by extrapolation. As the linear regression is not a good fit for all  $t_c$  (Fig. 5), the quality of the fit was measured with  $\chi^2$  and the result with minimal  $\chi^2$  was selected. The method works well for small amounts of intrinsic noise. A intrinsic noise with a standard deviation of 1% (as compared to the stimulus standard deviation) was estimated as 1.25% ( $t_c$ =600 ms, shown in 6B); an actual value of 5% was estimated as 6%, 10% was estimated as

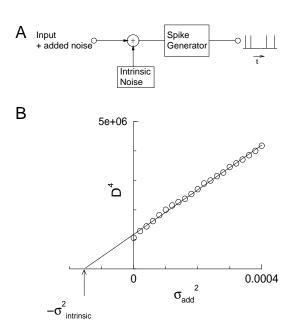


Figure 6: Using the distance to estimate the intrinsic noise of a cell. A: Model of the cell. The intrinsic noise in the cell is assumed to be additive to the input. B: The distance is plotted versus the variance of noise added to the stimulus. By adding noise the distance to the original response increases (circles). Note that at zero added noise, the distance is non-zero as the cell will not reproduce the exact same spike train due to the presence of the intrinsic noise. Extrapolation yields an estimate for the intrinsic noise.

12.6%, and 20% was estimated as 33%. Thus the method slightly overestimates the intrinsic noise. At higher levels of either added or intrinsic noise, the fitting deteriorates as the linear relation between  $\sigma^2$  and  $D^4$  gets higher order corrections. Nevertheless, we obtain a reasonable estimate for the intrinsic noise which is otherwise hard to access.

## 4 Conclusion

We have introduced a distance measure that computes the dissimilarity between two spike trains. To calculate the distance, filter both spikes trains and calculate the integrated squared difference of the two trains. The simplicity of the distance allows for an analytical treatment of simple cases. Numerical implementation is straightforward and fast.

The distance interpolates between, on the one hand, counting non-coincident spikes and, on the other hand, counting the squared difference in total spike count. In order to compare spike trains with different rates, total spike count can be used (large  $t_c$ ). However, for spike trains with similar rates, the difference in total spike number is not useful and coincidence detection is sensitive to noise. Instead, intermediate values of  $t_c$ , somewhat longer than the membrane time constant, are optimal.

The distance uses a convolution with the exponential function. This has an interpretation in physiological terms. Indeed, among other distances (see Introduction) our distance does not seem the most unlikely one to be implemented physiologically. For short and medium  $t_c$  the convolution can be interpreted as PSPs in a higher order neuron. For longer  $t_c$ , slower second messenger or calcium induced currents seem more appropriate. It would be interesting to see if such detection schemes are implemented biologically.

As an alternative measure, one could convolve the spikes with a square window. In that case the situation becomes somewhat similar to binning followed by calculating the Euclidean distance between the number of spikes in the bins. But in standard binning the bins are fixed on the time axis, therefore two different spike trains yield identical binning patterns as long as spikes fall in the same bin. However, with the proposed distance (convolving with either square or exponential) this does not happen; the distance is zero only if the two spike trains are fully identical (assuming  $t_c$  is finite).

The distance squared is related to the distance measure introduced by Victor and Purpura (Victor and Purpura 1996, Victor and Purpura 1997). One difference with this work is that their displacement distance was linear in the time difference, although they did suggest the use of an exponential displacement distance, Eq.(8). Another difference is that the distance introduced here is explicitly embedded in Euclidean space, which makes it less general but easier to analyze than the Victor and Purpura distance.

Interestingly, the distance is related to stimulus reconstruction techniques, where convolving the spike train with the spike triggered average yields a first order reconstruction of the stimulus (Rieke et al. 1996). Here the exponential corresponds roughly to

the spike triggered average and the filtered spike trains correspond to the stimulus (the exponentials are now attached to the other side of the spikes but that does not change the distance). The distance thus approximately measures the difference in the reconstructed stimuli, see Eq.(3). This might well explain the linearity of the measure for intermediate  $t_c$ . It also suggests that the distance measure might be refined by using the actual spike triggered average instead of an exponential.

A possible application for the distance measure is the insect olfactory system which uses a timing based code to distinguish between different odors (MacLeod et al. 1998). There it was shown, using the Victor and Purpura distance, that information was encoded in the temporal structure of the spike train, but not in the mean rate. Another application is the measurement of the intrinsic noise of a neuron or network, which is possible because the distance varies smoothly as noise is added to the input. For sensory systems stimulation with "natural" noisy stimuli has become quite common. Although natural stimuli are relevant in determining the system's response, the characterization of the noise in the system is less straightforward (Reich, Victor, Knight, Ozaki and Kaplan 1997). Measuring the intrinsic noise could be helpful. We stress that the intrinsic noise is a quantity which is otherwise difficult to measure experimentally. For instance, measurements of subthreshold fluctuations in the membrane potential fail to detect noise in the spike generator itself. By adding noise to the stimulus one can determine this intrinsic noise, which gives an effective description of the neuron's variability.

# References

- Geisler, W. S., Albrecht, D. G., Salvi, R. J. and Saunders, S. S. (1991). Discrimination performance of single neurons: rate and temporal information, *J. Neurophysiol.* **66**: 334–362.
- Gerstein, G. L. and Mandelbrot, B. (1964). Random walk models for the spike activity of a single neuron, *Biophys. J.* **4**: 41–68.
- Kistler, W. M., Gerstner, W. and van Hemmen, J. L. (1997). Reduction of the Hodgkin-Huxley equations to a single variable threshold model, *Neural Comp.* **9**: 1015–1046.
- Lu, Z.-L. and Dosher, B. A. (1999). Characterizing human perceptual inefficiencies with equivalent internal noise, *J. Opt. Soc. Am. A* **16**: 764–778.
- MacLeod, K., Backer, A. and Laurent, G. (1998). Who reads temporal information contained across synchronized and oscillatory spike trains?, *Nature* **395**: 693–698.
- Pelli, D. G. (1990). The quantum efficiency of vision, *in* C. Blakemore (ed.), *Vision: Coding and Efficiency*, Cambridge, Cambridge, pp. 9–24.
- Reich, D. S., Victor, J. D., Knight, B. W., Ozaki, T. and Kaplan, E. (1997). Response variability and timing precision of neuronal spike trains in vivo, *J. Neurophysiol.* **77**: 2836–2841.

- Rieke, F., Warland, D., de Ruyter van Steveninck, R. and Bialek, W. (1996). *Spikes: Exploring the neural code*, MIT Press, Cambridge.
- Tuckwell, H. C. (1988). *Introduction to theoretical neurobiology*, Cambridge University Press, Cambridge.
- Victor, J. D. and Purpura, K. P. (1996). Nature and precision of temporal coding in visual cortex: a metric-space analysis, *J. Neurophysiol.* **76**: 1310–1326.
- Victor, J. D. and Purpura, K. P. (1997). Metric-space analysis of spike trains: theory, algorithms and application, *Network: Comput. Neural Syst.* **8**: 127–164.

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