

REVIEW ARTICLE

Machine learning in major depression: From classification to treatment outcome prediction

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Abstract

Aims: Major depression disorder (MDD) is the single greatest cause of disability and morbidity, and affects about 10% of the population worldwide. Currently, there are no clinically useful diagnostic biomarkers that are able to confirm a diagnosis of MDD from bipolar disorder (BD) in the early depressive episode. Therefore, exploring translational biomarkers of mood disorders based on machine learning is in pressing need, though it is challenging, but with great potential to improve our understanding of these disorders.

Discussions: In this study, we review popular machine-learning methods used for brain imaging classification and predictions, and provide an overview of studies, specifically for MDD, that have used magnetic resonance imaging data to either (a) classify MDDs from controls or other mood disorders or (b) investigate treatment outcome predictors for individual patients. Finally, challenges, future directions, and potential limitations related to MDD biomarker identification are also discussed, with a goal of offering a comprehensive overview that may help readers to better understand the applications of neuroimaging data mining in depression.

Conclusions: We hope such efforts may highlight the need for an urgently needed paradigm shift in treatment, to guide personalized optimal clinical care.

KEYWORDS

classification, machine learning, magnetic resonance imaging, major depressive disorder, review

1 | INTRODUCTION

Major depressive disorder (MDD) is a highly prevalent psychiatric disorder with a significant effect on quality of life and socioeconomic burden.¹ The diagnosis of MDD often depends on criteria from the Diagnostic and Statistical Manual of Mental Disorders (DSM) and treatment response.² Due to the overlapping phenotypes across mental disorders as well as the heterogeneity within disorders such as MDD, clinical diagnoses are often not as well-defined as in research protocols. Consequently, patients with mood disorder sometimes have to endure the wrong drug trial or multiple

trials before receiving a final diagnosis.³ For situations in which the DSM classification is unclear and the subjective clinical impression is confusing, an effective diagnostic tool using, for example, objective brain imaging measurements is greatly needed.

Neuroimaging provides noninvasive measurements of brain function and structure, which can serve as a powerful tool for investigating discriminative biomarkers.^{4,5} Specifically, brain neuroanatomy is intrinsically complex and heterogeneous, which further complicates functional connectivity in patients with mental illnesses.⁶ Considering the high-dimensional imaging data quite often includes a limited number of samples, determining an effective and

optimal approach to diagnose mood disorder is particularly challenging.⁷ Studies discriminating major depressive disorders from healthy control (HC) or other mood disorders have been performed using several neuroimaging techniques, including magnetic resonance imaging (MRI), positron emission tomography (PET), magneto-encephalography (MEG), and electro-encephalography (EEG).^{8,9} Among which, MRI-related techniques such as functional MRI (fMRI), structural MRI (sMRI), and diffusion MRI (diffusion tensor images, DTI) show benefits of providing multiple perspective on brain function, structure, and their connectivity maps. These diverse brain imaging characteristics offer a great opportunity for researchers to unravel the secrets of the complex neuromechanism underlying depression.^{10–12} Beyond the group-level analyses which are often performed,^{13–16} there has been growing interest in using machine-learning (ML) techniques to identify phenotypes in a way that is clinically meaningful and feasible for translation into clinical diagnosis or prognosis,^{17,18} for example, (a) to predict response to currently available treatments or (b) to identify more specific targets for novel interventions.^{19,20}

In this selective review, we focus on machine-learning-based classification and prediction studies of MDD which utilize features derived from MRI data. First, based on a specific screening method, we selected 63 MRI-based machine-learning articles with MDD samples and surveyed the popular machine-learning methods implemented in these studies. Next, we highlight some representative studies on mood disorder discrimination, for example, MDD vs bipolar disorder (BD), and individualized prediction of treatment outcomes for MDD. Common biases are discussed and suggestions are provided. Finally, we discussed future directions for potential biomarker identification of MDD disorders. Approaches of mining big data focusing on classification and treatment strategies which are based on biological information rather than the clinical manifestation have the greatest potential to move the field forward.

2 | RESEARCH OVERVIEW

2.1 | Screening method

Studies were included if they focused on classification (including treatment prediction) between individuals with MDD and healthy controls (or other brain disorders) using machine-learning methods and employed magnetic resonance imaging as the data acquisition access. Figure 1I shows the screening method diagram called PRISMA (Preferred Reporting Items for Systematic Reviews and Meta-Analyses).²¹ Relevant articles were identified from searches in PubMed covering publications between January 2000 and December 2017, using the search terms, “depress*,” “MDD,” “MRI,” “fMRI,” “sMRI,” “DTI,” “magnetic resonance imaging,” “neuroimaging,” “classif*,” “diagno*,” “predict*,” “distinguish*,” “discriminat*,” “machine learning,” both in isolation and in combination. A total of 2045 articles were identified by the above search. Then, additional articles were identified through the reference lists of these papers to ensure

that no studies of significance were omitted from this review, resulting in another 82 articles. After removing duplicates, 1980 articles remained. Furthermore, 1874 were excluded during screening of the title and abstract and a further 40 were excluded during full-text screening. Finally, 66 MDD studies were selected, and we summarize their main findings below.

2.2 | Summary of metrics

Figure 1 indicates several key aspects of our survey. The number of papers published on this topic in each year from 2000 to 2017 is displayed on Figure 1A. Obviously, the publication number keeps growing and increases sharply in 2017. Figure 1B indicates the number of studies fallen within different classification groups, for example, MDD vs HC or MDD subtypes. It is clear that MDD vs HC classification is the largest category, followed by MDD vs BD. Predictive studies on MDD treatment outcome occur less frequently than classification studies. Figure 1C shows the proportion of popular machine-learning methods used in these studies. Support vector machines (SVM) remain the most prevalent method choice, but other ML methods have also been applied to MDD such as gaussian process classifier (GPC), linear discriminant analysis (LDA), and decision tree (DT), as well as more recent deep learning models. Figure 1D demonstrates the distribution of reported accuracy for 5 ml methods; SVM performance shows a large variability, which may be due to different sample sizes, whereas some uncommon methods show promising performance for specific cases. Furthermore, the proportion of different MRI modalities as well as the reported accuracy of each modality are shown in Figure 1E,F. Most studies still focused on using features of fMRI and sMRI (22 resting-state fMRI; 18 task-related fMRI; 21 sMRI), while some studies have begun to explore the discriminating ability of DTI (8 DTI) in spite of applying multimodal MRI features in one study. On the whole, rsfMRI data exhibit higher accuracy than other modalities. Figure 1G illustrates the distribution of reported sample sizes for each cross-validation (CV) methods including leave-one-out CV (LOOCV), 10-fold CV or others, and almost all studies with LOOCV had sample size smaller than 100 while the studies with 10-fold CV had a bigger mean sample size. Note that there is one special case which uses LOOCV with the largest sample size in our survey.²² Figure 1H shows the overall accuracy against the total sample size used in studies. Most studies had a smaller sample size and only one had more than 700,²² which raises a urgent need for including larger sample sizes for the study of MDD in machine-learning studies.

2.3 | Machine-learning pipeline

Figure 1J summarizes the most common machine-learning pipeline of MDD diagnosis and prediction using MRI data. After data pre-processing, the pipelines vary greatly but typically include the following steps: feature reduction, model training, classification, and performance evaluation.

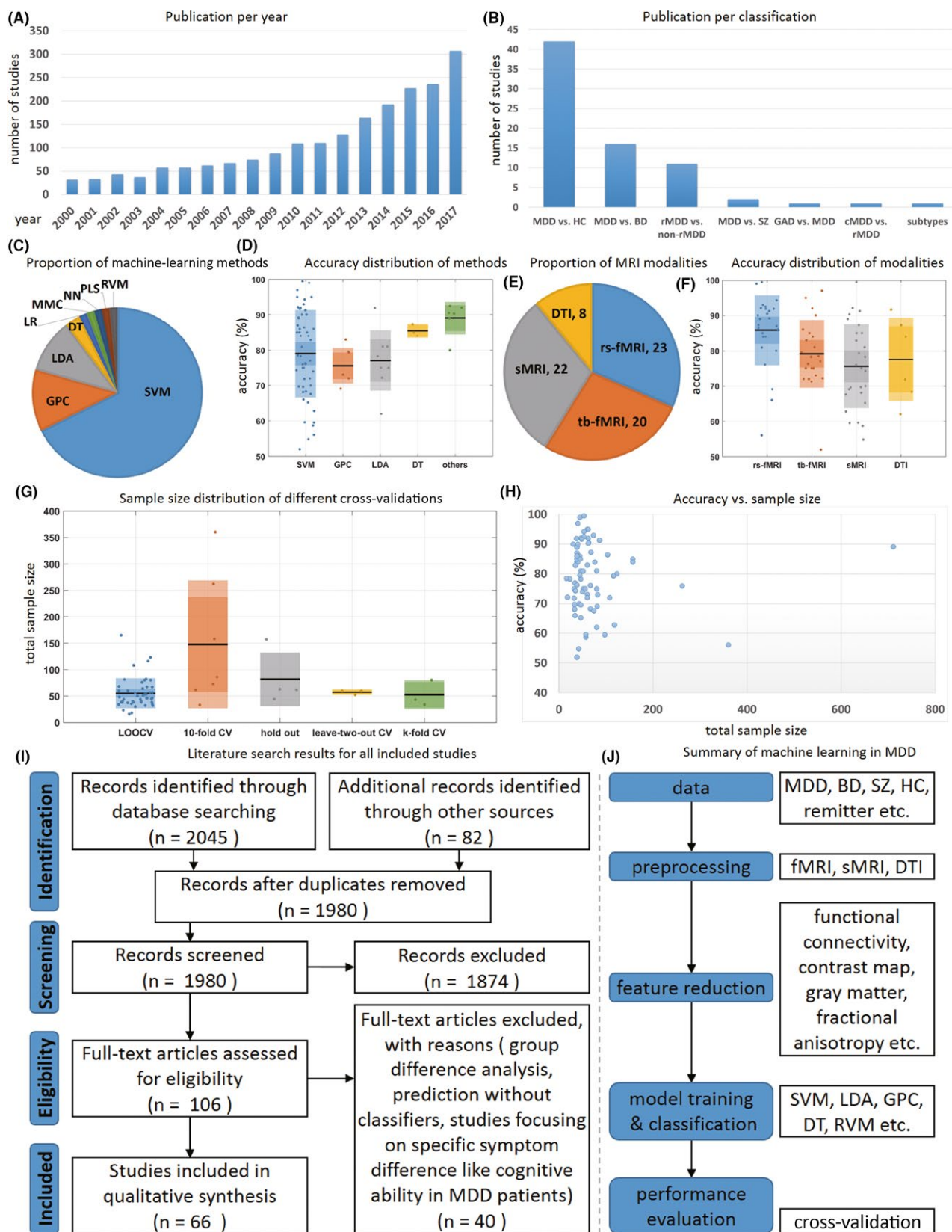


FIGURE 1 Visual summary of the selected MDD studies. A, Total number of papers before screening. B, Number of publications per group classification. C, Proportion of machine-learning methods used. D, Boxplot of accuracy based on five methods. E, Proportion of MRI modalities used. F, Accuracy based on modalities. G, Boxplot of sample size based on different cross-validation method. H, Scatter plot of overall reported accuracy vs the total sample size. I, Literature search results for each screening steps.²¹ J, Summary of steps in MRI machine learning

2.3.1 | Feature reduction

Feature reduction methods are essential to high-dimensional data which is a common problem in neuroimaging.²³ A limited number of the most relevant features warrant a more accurate classification model. These methods can be primarily categorized into feature selection and feature extraction. Feature selection is performed when supervised methods select the most discriminant features with the help of the labels of training data to reduce the noise. One strategy is to use prior knowledge to decrease dimensionality. Feature extraction occurs when methods project the original high-dimensional data into a lower dimension while maintaining its discriminative ability, and projection matrices are computed from training data. One typical example is principle component analysis (PCA). Both of these feature selection and feature extraction methods should only be conducted on training dataset (or the training groups assigned in cross-validation) to avoid biased results. Besides, some proposed approaches^{24,25} provide an intermediate solution by adopting geometric distance in feature space between different groups in the training data.²⁶

2.3.2 | Model training

In the training phase, for a supervised approach, a model is optimized using labeled data to find a discriminant “decision function” or “hyperplane” distinguishing between different groups (eg, depression patients and healthy controls).^{3,27} The parameters of the model are optimized to maximally discriminate one group from another. Cross-validation is usually used to generalize the training process. There are several types of cross-validation including k-fold, leave-one-out, and holdout. For k-fold CV, the training data are divided into k equal sized groups. Then, each one of k groups is treated as testing data and reiterated for k-iterations. The latter two techniques can be considered as variants of k-fold CV. Holdout approach is performed on data with large sample size ($k = 1$), while leave-one-out is used on data with small sample size ($k = \text{sample size}$).^{28,29}

2.3.3 | Classification

In the classification phase, the trained model is used to predict the label for new, previously unseen observations. For an unbiased generalization, it is important that the testing data do not overlap with training data.³⁰ The new data have to be preprocessed in the same way as the training data, and the same feature reduction method is applied with optimized parameters obtained from the training phase. In cases where independent testing data are not available due to limited samples, a nested cross-validation framework can be conducted to estimate the performance of the model.^{31–35} The most commonly used classifier in our survey is SVM because of its promising results in neuroimaging.³⁶

2.3.4 | Performance evaluation

The performance of classification-based algorithms can be described by accuracy, sensitivity, specificity, and receiver operating

characteristic (ROC) curve (sensitivity as a function of 1-specificity). Accuracy helps evaluate how accurately the model classifies test data. Sensitivity (or recall) refers to the proportion of true positives correctly identified (eg, percentage of true depression patients identified as MDD). In contrast, specificity refers to the proportion of true negatives correctly identified (eg, percentage of healthy people identified as HC). ROC curve illustrates the overall performance of method, usually summarized by the area under the curve (AUC). A confusion matrix, which is an $n \times n$ matrix for n labels with one side representing actual labels and the other representing predicted labels, can be useful when group of labeled data is more than two.³⁷ The confusion matrix also provides information relevant for imbalanced data and computing other performance measures such as precision (positive predictive value), F1-score (harmonic mean of precision and recall), and G-mean (geometric mean of precision and recall).³⁸ For imbalanced sample size data, balanced sensitivity (recall), specificity, and precision are more desirable than higher overall accuracy and thus such measures are preferred for evaluating the classifier in this case. Other ways of reporting results for imbalanced data include the F1-score and G-mean which help evaluate the performance of the results.

3 | MACHINE LEARNING IN MDD

Machine learning is defined as a group of methods that learn from empirical data to develop training models and make accurate classification from new data.³⁹ Its advantages in MDD are not confined to diagnosis, but also allow for the prediction of future disease progression, of which the most salient advantage one is its applicability to individual-level analysis. Table 1 summarizes various aspects of 66 selected studies.^{3,18–20,22,27,40–99} Most of these works aim at developing computational approaches to discriminate MDD from controls or mood disorder subtypes and trying to develop tools to integrate imaging measurements into clinical practice.

3.1 | Highlighted research

3.1.1 | Classification with brain networks in MDD

A number of studies used graph theory approaches^{43,45,46,82} to highlight the disrupted functional and structural brain networks in depression. These connectome-based biomarkers also provide new opportunities to redefine the diagnosis of depression and improve treatment measures by providing important knowledge about the biological mechanisms. Here, we summarize some of the key findings related to functional and structural brain networks in depression. In ref.¹⁰⁰, a review enumerated various brain network features, including altered regional and connectivity patterns of various MRI modalities in depression: ROI-based and voxel-based analysis (fMRI), regional betweenness and degree centralities (sMRI), and white matter structural connectivity (DTI). Reference⁸⁶ investigated the whole-brain resting-state functional connectivity patterns of

TABLE 1 Review of classification studies related to major depressive disorders

References	Subjects	Feature	Method	Cross-validation	Accuracy
Classification					
Rubin-Falcone et al (2017) ⁴⁰	BD = 26, MDD = 26	GM (sMRI)	SVM	Leave-two-out CV	75.0%
Deng et al (2017) ⁴¹	BD = 31, MDD = 36	FA (DTI)	SVM	LOOCV	68.3%
Gao et al (2017) ³	BD = 37, MDD = 36	Spatial independent components (rsfMRI)	SVM	10-fold CV	93.0%
Jing et al (2017) ⁴²	cMDD = 19, rMDD = 19, HC = 19	Hurst exponent (rsfMRI)	SVM	LOOCV	87.0% (cMDD vs HC), 84.0% (rMDD vs HC), 89.0% (cMDD vs rMDD)
Yoshida et al (2017) ⁴³	MDD = 58, HC = 65	FC (rsfMRI)	PLS	LOOCV	80.0%
Li et al (2017) ⁴⁴	BD = 22, MDD = 22	Degree centrality (rsfMRI)	SVM	LOOCV	86.0%
Zhong et al (2017) ⁴⁵	MDD = 29, HC = 33 (1st sample); MDD = 46, HC = 57 (2nd sample)	FC (rsfMRI)	SVM	LOOCV	91.9% (1st sample), 86.4% (2nd sample)
Wang et al (2017) ⁴⁶	MDD = 31, HC = 29	FC (rsfMRI)	SVM	LOOCV	95.0%
Schnyer et al (2017) ⁴⁷	MDD = 25, HC = 25	FA (DTI)	SVM	LOOCV	74.0%
Sundermann et al (2017) ⁴⁸	MDD = 180, HC = 180	FC (rsfMRI)	SVM	10-fold CV	45.0%~56.1%
Bhaumik et al (2017) ⁴⁹	MDD = 38, HC = 29	FC (rsfMRI)	SVM	LOOCV	76.1%
He et al (2017) ⁵⁰	BD = 13, MDD = 40, HC = 33	Functional network connectivity (rsfMRI), GM(sMRI)	SVM	10-fold CV	91.3% (three groups), 99.0% (BD vs MDD)
Bürger et al (2017) ⁵¹	BD = 36, MDD = 36, HC = 36	Contrast maps (task fMRI)	SVM, GPC	LOOCV	72.0%
Hilbert et al (2016) ⁵²	GAD = 19, MDD = 14, HC = 24	GM (sMRI)	SVM	LOOCV	58.7% (GAD&MDD vs HC), 68.1% (GAD vs MDD)
Drysdale et al (2016) ²²	MDD = 333(4 biotypes), HC = 378	FC (rsfMRI)	SVM	LOOCV	89.2%
Sankar et al (2016) ⁵³	MDD = 23, HC = 20	GM, WM (sMRI)	SVM	5-fold CV	70.0%
Frangou et al (2016) ⁵⁴	BD = 30, MDD = 30	Contrast maps (task fMRI)	GPC	leave-two-out CV	73.1%
Ramasubbu et al (2016) ⁵⁵	MDD = 15, HC = 19	Spatial independent components (rsfMRI)	SVM	5-fold CV	66.0%
Yang et al (2016) ⁵⁶	MDD = 16, HC = 16	Contrast maps (task fMRI)	SVM	LOOCV	75.0%
Rive et al (2016) ⁵⁷	MDDr = 23, BDr = 26, MDDd = 22, BDd = 10	GM (sMRI), Spatial independent components (rsfMRI)	GPC	LOOCV	69.1%
Jie et al (2015) ²⁷	BD = 21, MDD = 25	GM (sMRI), fALFF (rsfMRI)	SVM	LOOCV	92.1%
Foland-Ross et al (2015) ⁵⁸	MDD = 18, HC = 15	CTH (sMRI)	SVM	10-fold CV	69.7%
Sacchet et al (2015) ⁵⁹	BD = 40, MDD = 57, HC = 61	GM (sMRI)	SVM	10-fold CV	59.5% (BD vs MDD), 62.8% (MDD vs HC)
Sacchet et al (2015) ⁶⁰	MDD = 14, HC = 18	Graph metric of WM connectivity (DTI)	SVM	LOOCV	71.9%
Sato et al (2015) ⁶¹	MDD = 25, HC = 21	Contrast maps (task fMRI)	LDA	LOOCV	78.3%

(Continues)

TABLE 1 (Continued)

References	Subjects	Feature	Method	Cross-validation	Accuracy
Johnston et al (2015) ⁶²	MDD = 20, HC = 21	GM (sMRI)	SVM	LOOCV	85.0%
Johnston et al (2015) ⁶³	MDD = 19, HC = 21	Contrast maps (task fMRI)	SVM	LOOCV	97.0% (hippocampus), 84.0% (striatum)
Koutsouleris et al (2015) ⁶⁴	MDD = 104, SZ = 158	GM (sMRI)	SVM	10-fold CV	76.0%
Shimizu et al (2015) ⁶⁵	MDD = 31, HC = 31	Contrast maps (task fMRI)	gL-ASSO, SVM	10-fold CV	92.0% (gLASSO), 95.0% (SVM)
Fung et al (2015) ⁶⁶	BD = 16, MDD = 19	CTH and surface area (sMRI)	SVM	LOOCV	74.3%
Rosa et al (2015) ⁶⁷	MDD = 19, HC = 19	FC (task fMRI)	SVM	LOOCV	85.0%
Patel et al (2015) ⁴⁸	MDD = 33, HC = 35	rsfMRI, sMRI, DTI	DT	LOOCV	87.3%
Redlich et al (2014) ⁶⁸	BD = 58, MDD = 58	GM (sMRI)	GPC	LOOCV	79.3%
Cao et al (2014) ⁶⁹	MDD = 39, HC = 37	FC (rsfMRI)	SVM	LOOCV	84.0%
MacMaster et al (2014) ⁷⁰	BD = 14, MDD = 32	GM (sMRI)	LDA	N/A	81.0%
Zeng et al (2014) ⁷¹	MDD = 24, HC = 29	FC (rsfMRI)	MMC	LOOCV	92.5% (clustering), 92.5% (classification)
Rondina et al (2014) ⁷²	MDD = 30, HC = 30	Voxel intensity (task fMRI)	SVM	leave-two-out CV	72.0%
Guo et al (2014) ⁷³	MDD = 36, HC = 27	FC (rsfMRI)	NN	hold out	90.5%
Serpa et al (2014) ⁷⁴	BD = 23, MDD = 19, HC = 38	GM, WM, and ventricular RAVENS maps (sMRI)	SVM	LOOCV	54.8% (BD vs MDD), 59.6% (MDD vs HC)
Habes et al (2013) ⁷⁵	MDD = 9, HC = 9	Contrast maps (task fMRI)	LDA	LOOCV	72.2%
Wei et al (2013) ⁷⁶	MDD = 20, HC = 20	Spatial independent components (rsfMRI)	SVM	LOOCV	90.0%
Grotegerd et al (2013) ⁷⁷	BD = 22, MDD = 22	Contrast maps (task fMRI)	GPC	LOOCV	79.6%
Yu et al (2013) ⁷⁸	MDD = 19, SZ = 32	FC (rsfMRI)	SVM	LOOCV	80.9%
Modinos et al (2013) ⁷⁹	MDD = 17, HC = 17	Contrast maps (task fMRI)	SVM	LOOCV	77.0%
Ma et al (2013) ⁸⁰	MDD = 19, HC = 18	ReHo (rsfMRI)	LDA	LOOCV	91.9%
Grotegerd et al (2013) ⁸¹	MDD = 10, BD = 10, HC = 10	Contrast maps (task fMRI)	SVM, GPC	LOOCV	90.0%
Fang et al (2012) ⁸²	MDD = 22, HC = 26	Anatomical connectivity (DTI)	SVM	LOOCV	91.7%
Mwangi et al (2012) ⁸³	MDD = 30, HC = 32	GM (sMRI)	RVM	hold out	90.3%
Lord et al (2012) ⁸⁴	MDD = 22, HC = 22	FC (rsfMRI)	SVM	hold out	99.0%
Liu et al (2012) ⁸⁵	TRD = 18, TSD = 17, HC = 17	GM, WM (sMRI)	SVM	LOOCV	82.9%
Zeng et al (2012) ⁸⁶	MDD = 24, HC = 29	FC (rsfMRI)	SVM	LOOCV	94.3%
Mourão-Miranda et al (2011) ⁸⁷	MDD = 19, HC = 19	Contrast maps (task fMRI)	SVM	LOOCV	52.0% (true positive)
Hahn et al (2011) ⁸⁸	MDD = 30, HC = 30	Contrast maps (task fMRI)	GPC	LOOCV	83.0%
Nouretdinov et al (2011) ⁸⁹	MDD = 19, HC = 19	Contrast maps (task fMRI)	SVM	LOOCV	76.3%

(Continues)

TABLE 1 (Continued)

References	Subjects	Feature	Method	Cross-validation	Accuracy
Costafreda et al (2009) ⁹⁰	MDD = 37, HC = 37	GM (sMRI)	SVM	LOOCV	67.6%
Fu et al (2008) ⁹¹	MDD = 19, HC = 19	Contrast maps (task fMRI)	SVM	LOOCV	86.0%
Prediction					
Jiang et al (2017) ¹⁹	rMDD = 27, non-rMDD = 11	GM (sMRI)	LR	LOOCV	89.0%
Redlich et al (2016) ²⁰	MDD responder = 13, non-responder = 10	GM (sMRI)	SVM	LOOCV	78.3%
Lythe et al (2015) ⁹²	rMDD = 31, non-rMDD = 25	FC (task fMRI)	LDA	LOOCV	75.0%
Korgaonkar et al (2015) ⁹³	rMDD = 54, non-rMDD = 103	Volume (sMRI), FA (DTI)	DT	hold out	85.0% (sMRI), 84.0% (DTI)
Williams et al (2015) ⁹⁴	MDD responder = 48, non-responder = 32	Contrast maps (task fMRI)	LDA	LOOCV	75.0% (happy), 81.0% (sad)
Schmaal et al (2015) ⁹⁵	rMDD = 23, non-rMDD = 59	Contrast maps (task fMRI)	GPC	LOOCV	73.0%
van Waarde et al (2014) ⁹⁶	rMDD = 25, non-rMDD = 20	Spatial independent components (rsfMRI)	SVM	LOOCV	84.0% (sensitivity), 85.0% (specificity)
Korgaonkar et al (2014) ⁹⁷	rMDD = 37, non-rMDD = 43	FA (DTI)	LDA	k-fold CV	62.0%
Gong et al (2011) ⁹⁸	rMDD = 23, non-rMDD = 23	GM, WM (sMRI)	SVM	LOOCV	69.6% (GM), 65.2% (WM)
Costafreda et al (2009) ⁹⁹	rMDD = 9, non-rMDD = 7	Contrast maps (task fMRI)	SVM	LOOCV	71.0% (sensitivity), 86.0% (specificity)

BD, bipolar disorder; MDD, major depressive disorder; cMDD, current MDD; rMDD, remitted MDD; GAD, generalized anxiety disorder; SZ, schizophrenia; TRD, treatment-resistant depression; TSD, treatment-sensitive depression; GM, gray matter; MRI, magnetic resonance imaging; DTI, diffusion tensor images; FC, functional connectivity; WM, white matter; fALFF, fractional amplitude of low-frequency fluctuation; CTH, cortical thickness; ReHo, regional homogeneity; GPC, gaussian process classifier; LDA, linear discriminant analysis; gLASSO, group least absolute shrinkage and selection operator; CV, cross-validation; LOOCV, leave-one-out cross-validation; FA, fractional anisotropy; RAVENS, regional analysis of volumes examined in normalized space; LR, linear regression; PLS, partial least squares regression; DT, decision tree; MMC, maximum margin clustering; NN, neural network; RVM, relevance vector machine; BDd, bipolar disorder, depressed state; BDr, bipolar disorder, remitted state; MDDd, major depressive disorder, depressed state; MDDr, major depressive disorder, remitted state.

depressed patients to identify major depressive individuals from healthy controls and achieved 100% sensitivity. The most discriminating functional connections were located within or across the default mode network, affective network, visual cortical areas, and cerebellum, which may play important roles in the pathological mechanism of this disorder.

3.1.2 | Prediction of treatment response in MDD

Altered network activity at rest has been explored as a potential biomarker for predicting treatment outcomes. As shown in ref. ²², four distinct MDD neurophysiological biotypes, characterized by distinct patterns of limbic and frontostriatal functional connectivity, were defined using fMRI. These biotypes were associated with distinct profiles of clinical symptoms; for example, biotype 1, which responded best to repetitive transcranial magnetic stimulation (rTMS) therapy, was associated with high levels of fatigue and low anhedonia. Similarly, electroconvulsive therapy (ECT) is a popular treatment for depression patients. Several studies have explored biomarkers that potentially predict the response to ECT.

One of the studies investigated whether gray matter (GM) volume changes are able to predict ECT response. Support vector regression was performed before treatment and supplemented with univariate analysis of the Hamilton Depression Rating Scale score (HDRS), yielding a successful prediction of ECT response and a significant prediction of relative reduction in the HDRS.²⁰ Another study predicted post-ECT depressive remission status using pre-ECT GM in MDD patients and validated in two independent datasets. Six GM networks were identified as predictors of ECT response, achieving accuracy of 89%, 90% and 86% for remission prediction in three independent datasets.¹⁹

3.2 | Common machine-learning challenges in MDD study

Studies involving a combination of MRI and pattern recognition techniques to explore biomarkers of depression have grown substantially in recent years. Such methods can accurately discriminate depressed subjects from healthy controls^{43,45–49,88,89,91} and predict treatment response.^{19,20,90,92} In

our survey, there are more studies focused on classification (53 studies) than treatment response prediction (10 studies). To the best of our knowledge, the number of articles that use machine-learning methods for classifying depression is limited,¹⁰¹ and many of these methods have not been integrated into a clinical application. We believe the main reason is the heterogeneity of imaging data including data collection, scanning parameters, and processing methods which hampers generalization to other datasets. This makes it difficult to draw comparisons based on the results.

3.2.1 | Small sample size

The small sample size is a universal problem faced by most studies of depression as reported till now, and it is hence not easy to draw definite conclusions about the diagnostic value of neuroimaging at the individual level, although several MDD studies working on thousands of samples are still ongoing. Given the difficulty of recruiting patients, the limitation of a small sample size is quite understandable. This problem is naturally difficult and common in machine-learning methodologies, but the sample size is still miniscule in comparison with other fields in which machine learning is used leading to several problems. There are a growing number of repositories which address the broader issue of small sample sizes within neuroimaging research,²² but these typically lack uniformity between contributing sites with respect to acquisition and processing parameters which may introduce bias to the aggregated data. As long as there is no common standard between different sites, performing machine-learning methods is limited to the available sample sizes.

3.2.2 | Feature reduction

Given the small sample sizes used by the past studies, a proper feature reduction method should be used to improve overall performance. Features used by past studies vary considerably by MRI modality, feature reduction method, and number and type of features. Despite this, various features in past studies seem to be useful in major depression, for example reduced activation in dorsolateral prefrontal areas^{3,18,43,46,48,50,82} and decreased gray matter volume in prefrontal cortex and subcortical systems.^{59,62,64,68,83,98} Group differences conducted on whole dataset were applied to select features in some studies,⁵⁰ but this may introduce bias into the feature selection step.^{102,103} There is not a direct relationship between statistical analysis and discrimination power as they are different criteria.¹⁰¹ As such valuable discriminatory information could be lost by discarding features based on group differences,^{104–106} better approaches should be introduced including recursive feature elimination (RFE),²⁷ minimum-redundancy maximum relevancy (mRMR),¹⁰⁷ and methods that learn the features contributing most to the accuracy of the model like least absolute shrinkage and selection operator (LASSO), elastic net and ridge regression.^{19,65}

3.2.3 | Overfitting

Overfitting can result in very good performance on training data, but very poor performance on testing data, and poor generalization to independent datasets,¹⁰⁸ which may be caused by small sample size with high-dimensional features^{32,109} and complex models with too many parameters. Neuroimaging applications in MDD unsurprisingly can also suffer from overfitting. And cross-validation is a common approach to control for overfitting. As mentioned above, the proper type of CV should be selected based on the data scale, as shown in Figure 1G.

3.2.4 | Classification methods and cross-validation

Almost all of the selected studies used SVM or its variant method as the primary classification method^{22,40–42,44–50,52,53,82,84,87,89–91,98} and use LOOCV for cross validation. The reason why SVM is the most popular choice among depression classification is because of its useful strengths on including a reliable theoretical foundation and its flexible response to high-dimensional data. Considering most neuroimaging studies are likely to be nonlinear, kernel SVM has been proposed to achieve better performance than the other methods for nonlinear depression classification.⁶⁵ Nevertheless, if the number of samples is significantly less than the number of features, it may be better to simply use the linear-learning-based method to avoid complexity and mitigate against overfitting.^{110,111} For cross validation, the LOOCV method provides more data to the training stage of learning method, which is associated with high variance, which may weaken generalization performance and lead to overfitting.^{112,113} According to our recent work, 10-fold CV provides a more stable performance across different data while LOOCV performance heavily depends on the used data.³

4 | FUTURE DIRECTIONS

Based on the discussion in the previous section of past studies, there are several potential directions to explore for future studies (Figures 2 and 3).

4.1 | Multi-cross-classification for large sample size and deep learning

The selection of appropriate learning methods is very important to accurately learn a classification framework. Some researchers have successfully realized this selection of methods as applied to other brain disorders.^{114–116}

Large sample size is of great importance for valid classification performance, but it is often not easy to collect large samples at one single site. To address this problem, multisite data sharing has been proposed which allows for cross-site classification of psychiatric disorders such as schizophrenia. In cross-site classification, the model is trained at one or several independent sites and tested at different

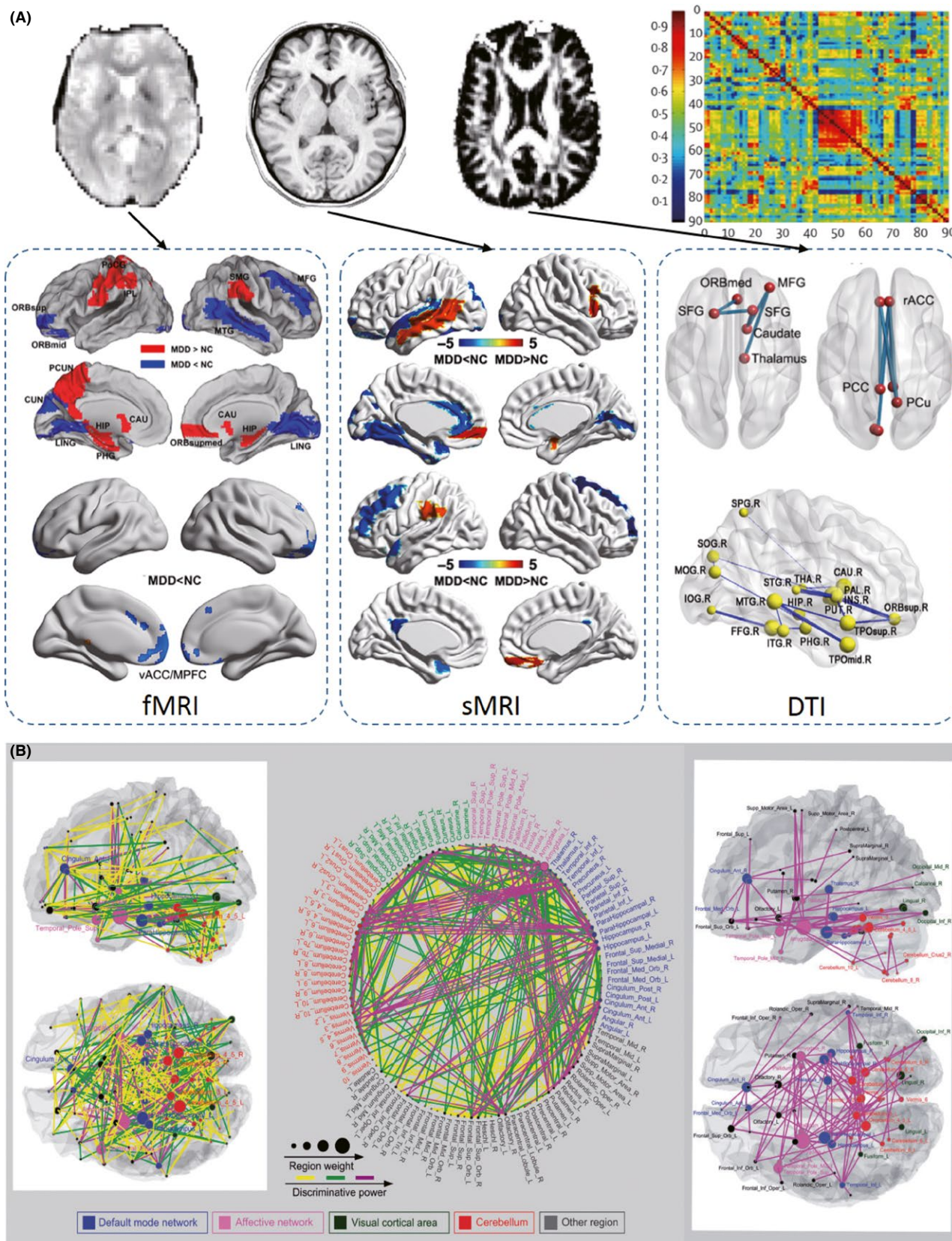
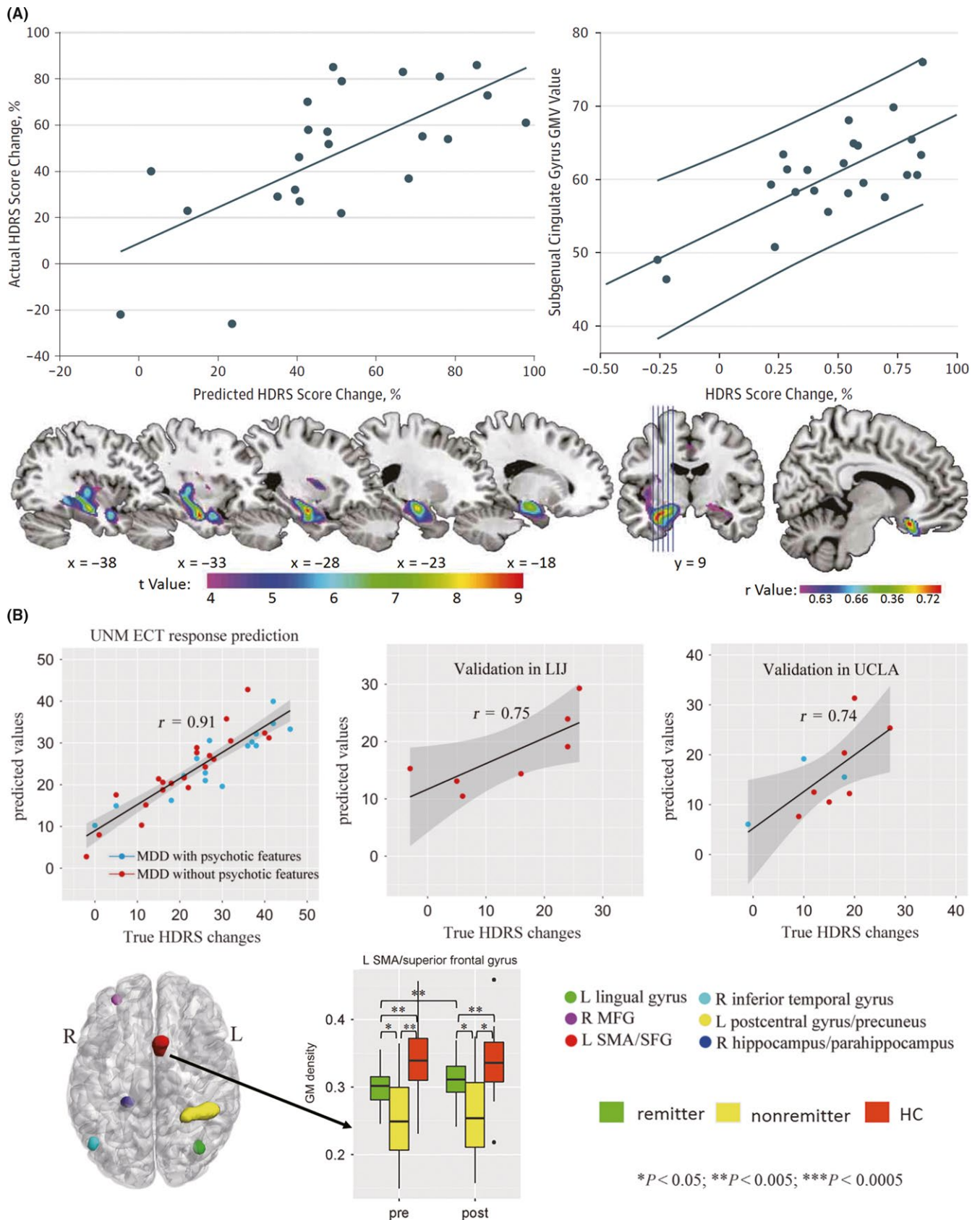


FIGURE 2 Brain network studies in MDD classification. A¹⁰⁰: Brain network construction with MRI and connectome architecture represented by a connectivity matrix. B⁸⁶: Region weights and distribution of 442 consensus functional connections identified by classification of MDD and HC demonstrated in sagittal and axial view (left) and in a circle graph (middle). Top 100 most discriminating consensus functional connections in sagittal and axial view (right). [A reproduced from ref. ¹⁰⁰; B reproduced from ref. ⁸⁶]



sites. As a significant machine-learning method for large multisite data, cross-classification can tackle the problem of overfitting and further provide potential biomarkers less specific to one certain site, which

will be more generalizable in clinical practice. Rozycki et al used advanced multivariate analysis tools and structural neuroimaging data of 941 participants from five sites to find neuroanatomical signature of

FIGURE 3 Predication studies in MDD. A²⁰: Positive association between predicted and true change in the Hamilton Depression Rating Scale (HDRS) score. Positive association between change in HDRS score and subgenual anterior cingulate volume before electroconvulsive therapy (ECT). Gray matter volume (GMV) increasing in the ECT group. Spatial map of correlated anterior cingulate volume. B¹⁹: Scatter plot of the predicted Δ HDRS (Hamilton Depression Rating Scale) with respect to their true values for three sites, extracting six identified pre-electroconvulsive therapy (ECT) gray matter (GM) regions in University of New Mexico (UNM) and using them as regressors for two independent cohorts: Long Island Jewish Health System (LIJ) and University of California at Los Angeles (UCLA). Six identified pre-electroconvulsive therapy (ECT) GM regions of interest (ROIs) as predictors of Δ HDRS in axial view. Longitudinal GM changes among remitters, nonremitters, and healthy controls of left supplementary motor area (SMA) and superior frontal gyrus (SFG). [A reproduced from ref. ²⁰; B reproduced from ref. ¹⁹]

patients with schizophrenia and establish cross-site classification with robust generalizability.¹¹⁴ Zeng et al proposed discriminant deep learning method using fMRI of 734 participants from seven sites to learn discriminating functional connections and achieve accurate prediction.¹¹⁵ Both of the studies conducted pooling classification and leave-site-out validation, and obtained promising classification results. Discriminating brain patterns were shared by all sites. Cross-site classification is still challenging, but shows promise for the future.

Another state of the art machine-learning method is deep learning, which has the ability to extract hidden information from high-dimensional data, and some researches have already show enhanced classification accuracies with neuroimaging data. For example, Kim et al adopt deep neural network (DNN) with L1-norm controlling weight sparsity in hidden layer for whole-brain resting-state FC pattern classification of schizophrenia vs HC.¹¹⁶ Zeng et al investigated cross-site classification with deep learning in schizophrenia for the first time.¹¹⁵ These methods may transfer to other neuropsychiatric disorders such as MDD to build diagnostic tools and provide better analysis about pathophysiology.

4.2 | Multimodal MRI in MDD

Although fMRI and sMRI biomarkers have been found to be associated with depression, there are additional studies that have shown the relevance of DTI biomarkers.^{41,47,58,93} Additionally, nonimaging measures have also been used in depression.¹¹⁷ Thus, it is important to study how multimodal MRI in conjunction with nonimaging features affects prediction models of depression.^{27,50} Each MRI modality represents different view of the brain, and data fusion capitalizes on the strengths of each modality and their inter-relationships in a joint analysis to unravel the pathophysiology of brain disease.^{117–119} Recent advances in data fusion^{120–122} increase our confidence in multimodal approaches and also provide insight into both anatomical and functional information.^{123–125} Often multimodal studies reveal information which may be missed by methods based on a single modality.¹²⁶ Some studies have already applied advanced multimodal fusion methods like multisite canonical correlation analysis with reference + joint independent component analysis (mCCA+jICA)¹¹⁹ and its variants¹¹⁷ in MDD associated analysis with promising classification performance.⁵⁰ In ref. ²⁷ jointly selected features from amplitude of low-frequency fluctuation (ALFF) and GM trained by the SVM classifier enable classifying MDD and BD at high accuracy based on the identified features (eg, dorsal lateral prefrontal cortex in GM). Data fusion methods

combined with machine learning are thus a promising direction for depression classification.

4.3 | Multiple classification and subtypes

Multiple classification can be performed via a pseudo multiclass strategy by applying a two-class algorithm either to separate pairs of depression subtypes or to separate different subtype from one other. An alternative approach for this problem is to apply clustering methods to label subjects as belonging to specific disease subtype clusters.²² Although abnormalities of major neuroanatomical regions and neural networks are common in one generalized category of disorders, prominently disturbed symptoms differ between subtypes, which have already been found in MDD¹²⁷ and BD.^{128,129} Differentiating a disorder sharing symptoms with other disorders is also one of the main challenges in psychiatry and neurology. It has been reported that such overlapping disorders include schizophrenia, bipolar, unipolar, and mood disorders. Classification with task-based fMRI has achieved good performance in distinguishing schizophrenia and bipolar disorder.^{130–132} Other studies also classify schizophrenia, bipolar and healthy controls with high accuracy using sMRI.^{59,64,133,134} So, multiple classification in depression is thought to be very promising but also challenging.²²

Besides, there are also some researches applying machine-learning methods to explore vulnerable biomarkers. In the field of MDD, Opel et al investigated gray matter alterations of healthy controls, MDD patients, healthy first-degree relatives of MDD and healthy individuals exposed to former childhood maltreatment using univariate analysis (t test) and pattern recognition approach (SVM) to conduct both group- and individual-level analyses. The classifier can successfully detect individuals with a risk of MDD and perform even better with the help of specific brain regions associated with MDD found by group-level analysis, showing the potential power in searching familial and environmental risk factors for MDD in the future.¹³⁵

4.4 | Large-scale datasets

Problems with data heterogeneity may be reduced through using large training datasets.^{32,109} In the past few years, several multiple center data repositories such as PGC, ENIGMA, UK Biobank, and others have been started, and they are all collaborative confederation with many working groups including major depression group. Despite some respective MDD group of these large consortium contains relatively smaller sample size, there are also marvelous achievements. For example, MDD workgroup has been a part of

the PGC since 2007, and now it covers over 100 000 people with depression. The PGC MDD group has published a paper¹³⁶ confronting the notably challenges in genetic dissection of MDD and keeps increasing sample size and expanding their studies.^{137–140} The ENIGMA MDD working group includes brain scans of around >5000 MDD patients and >9000 controls from 35 research samples of 14 different countries worldwide. Its primary aim is to identify imaging markers that robustly discriminate MDD patients from healthy controls cross-site with standardized image processing and statistical analysis protocols.^{141–144} More recently, a predictive analytics competition (PAC), a major depression classification challenge with the goal of automatic classification of patients suffering from major depression, and healthy individuals based on sMRI data have been carried out (<https://www.photon-ai.com/pac>). The training data of PAC contain labeled sMRI data of 759 MDD patients and 1033 normal controls from three different sites which are free to public. The unlabeled testing data of totally 448 individuals from three sites are also available. The winners of 2018 PAC competition achieved 65% accuracy on classifying MDD from HC. Another ongoing project named REST-meta-MDD in China also integrated multisite meta-analysis results from thousands of resting-state fMRI data of MDD and HC. We believe that the field of MDD can benefit a lot from similar machine-learning competitions and projects.

5 | CONCLUSIONS

The widespread availability of machine-learning methods combined with MRI data affords unprecedented opportunities to further deepen individual-level analysis of major depression and accelerate translation to clinical application. Approaches for combining machine-learning methods and MRI data are still largely at the exploratory stage. Classification models and features extracted from multiple modalities are irregular across different studies and this heterogeneity makes it harder to unearth optimal MRI modalities, features, and algorithm. Currently, the trend of combining machine learning approaches and MRI data in depression is drawing more attention due to the high potential and provides more information about the underlying brain regions which are involved. Though there are many challenges, but there is still huge potential for approaches which could leverage multimodal data types, brain connectomics, big data from different centers, subtype classification, and combination with clinical and genetic information.

CONFLICT OF INTEREST

The authors declare no conflict of interest.

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