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# Pretraining Deformable Image Registration Networks with Random Images

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## Introduction

**Background:** Deep learning-based image registration methods typically require large domain-specific datasets for effective generalization. Recent research indicates that training on randomly generated images may effectively replace domain-specific pretraining [1], improving efficiency and reducing the amount of required labeled medical data.

**Objective:** This study proposes a novel pretraining strategy using registration between random images as a proxy task to train deformable registration networks, aiming to enhance generalizability, reduce reliance on domain-specific data, and accelerate convergence.

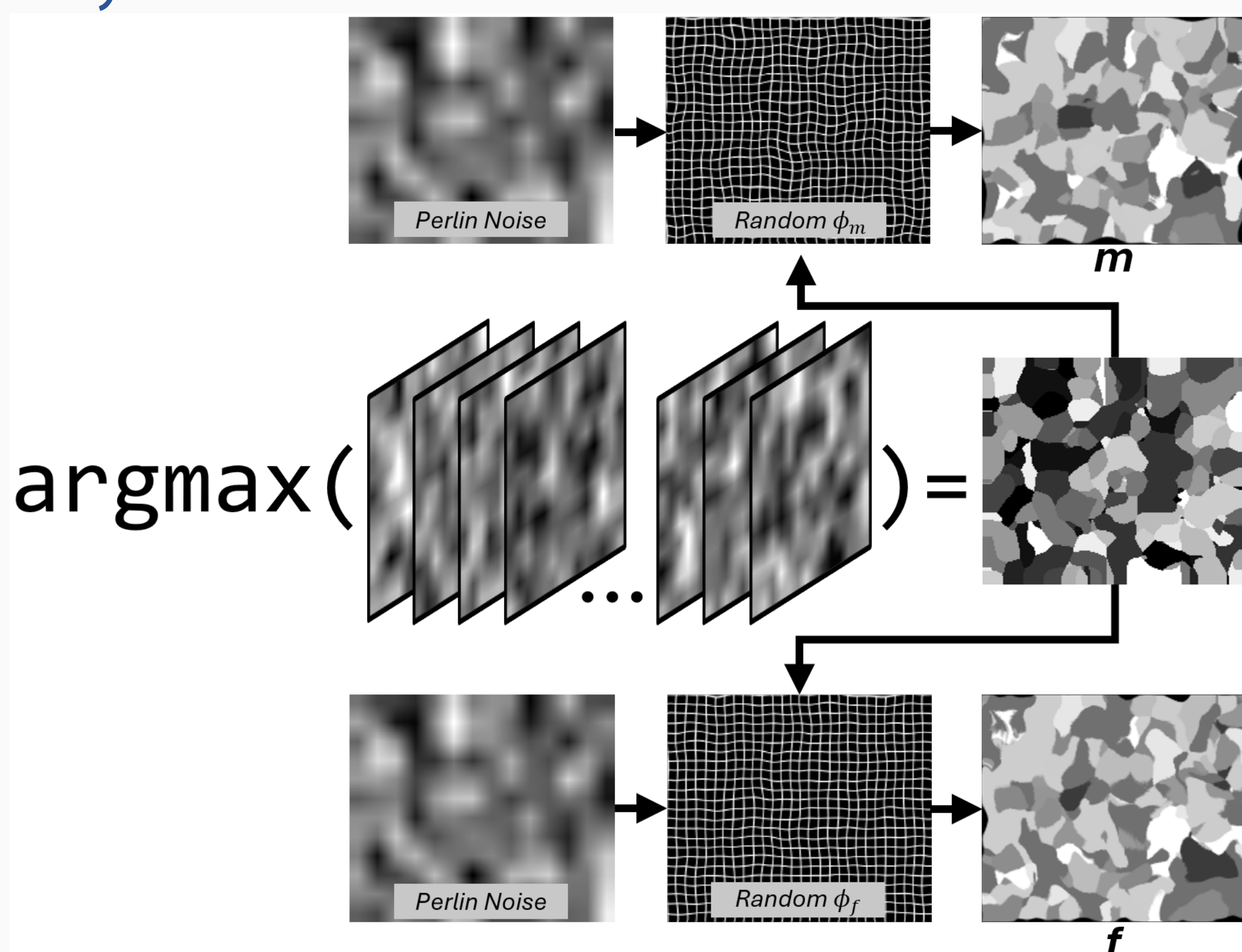
## Methods

### Proposed Pretraining Strategy:

Let  $m$  and  $f$  represent the moving and fixed images, respectively.

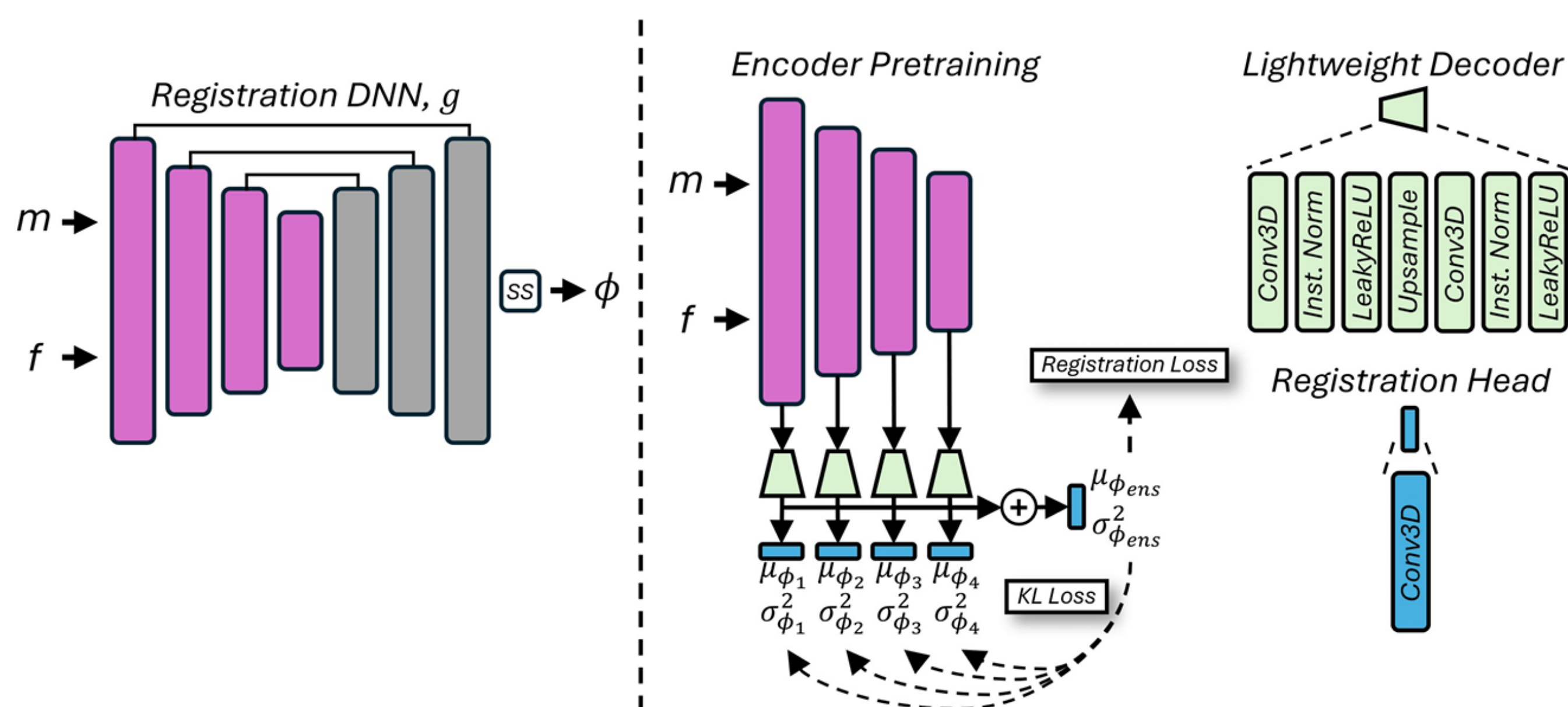
#### 1. Random Image Generation:

Multi-channel Perlin noise-generated random shapes **without** additional Gaussian noise or bias fields; diffeomorphic deformation fields applied to create random image pairs dynamically.



#### 2. Network Architecture:

We pretrain only the **encoder** of TransMorph [2] by pairing it with lightweight **temporary decoders** at multiple resolutions. These temporary decoders are discarded after pretraining. This asymmetric design, often used in computer vision [3], concentrates the learning of meaningful features within the encoder.



#### 3. Self-Distillation Strategy:

Ensemble-based method using KL-divergence between decoder outputs to enhance consistency and representation learning across layers.

#### 4. Loss Function for Pretraining:

Combines normalized cross-correlation (NCC) loss, diffusion regularizer, and KL-divergence-based self-distillation terms:

$$\mathcal{L}_{pretrain}(m, f) = \mathcal{L}_{NCC}(m \circ \mu_{\phi_{ens}}, f) + \lambda \|\nabla u_{ens}\|^2 + \eta \sum_{k \in K} \frac{1}{K} \mathcal{D}_{KL}(\mathcal{N}(\mu_{\phi_{ens}}, \sigma_{\phi_{ens}}^2) || \mathcal{N}(\mu_{\phi_k}, \sigma_{\phi_k}^2)),$$

## Methods (Cont.)

where the ensemble deformation field is represented by the mean  $\mu_{\phi_{ens}}$  and variance  $\sigma_{\phi_{ens}}^2$ , while  $\mu_{\phi_k}$  and  $\sigma_{\phi_k}^2$  are the estimates from the decoder at stage  $k$ .

### Experimental Setup:

- Datasets:** IXI brain MRI, comparison with deedsBCV [4], SynthMorph [1], and ConvexAdam [5].
- Training:** Pretrained for 50 epochs, fine-tuning with 1·NCC+1·Diffusion Reg. for 250 epochs.

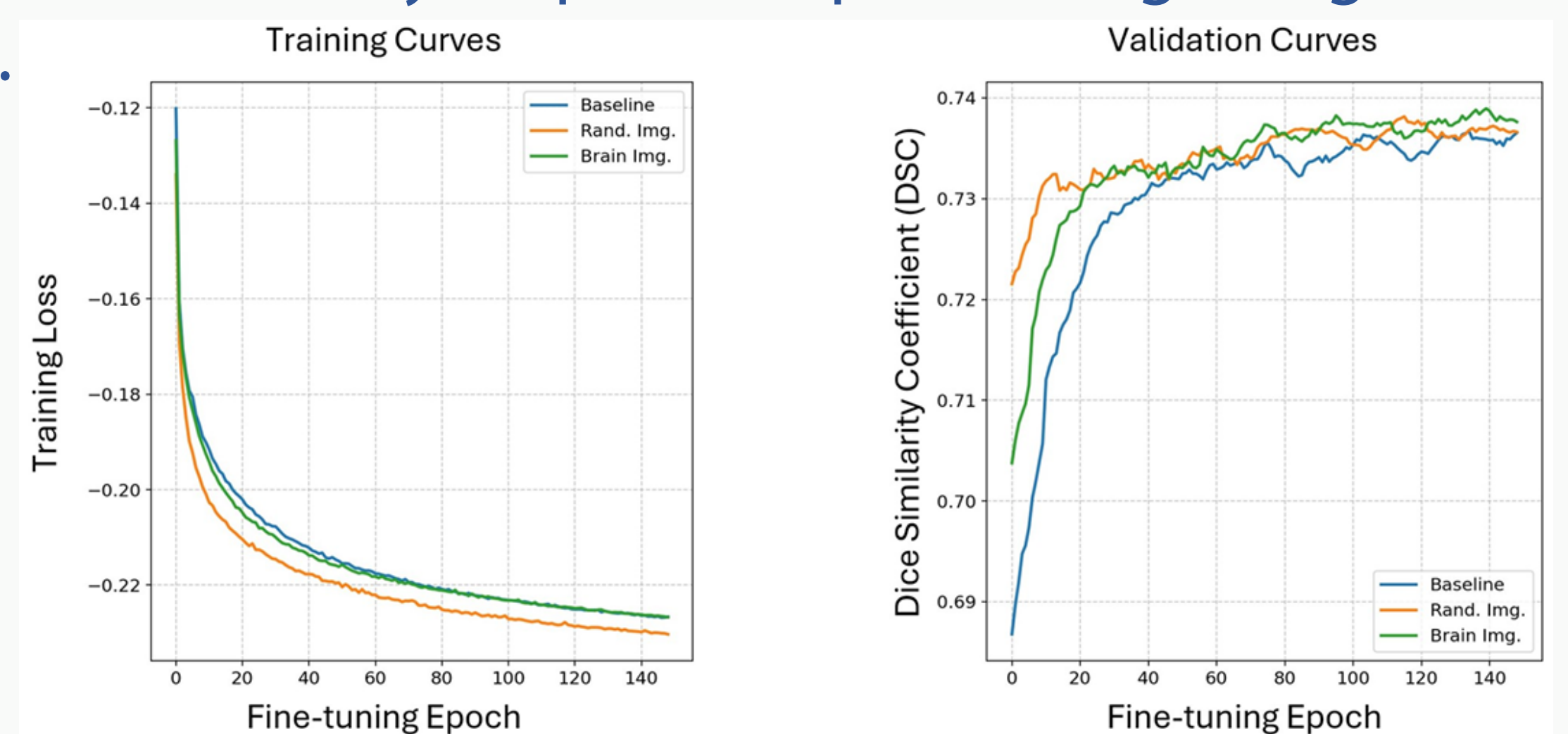
## Results

### Improved Registration Performance:

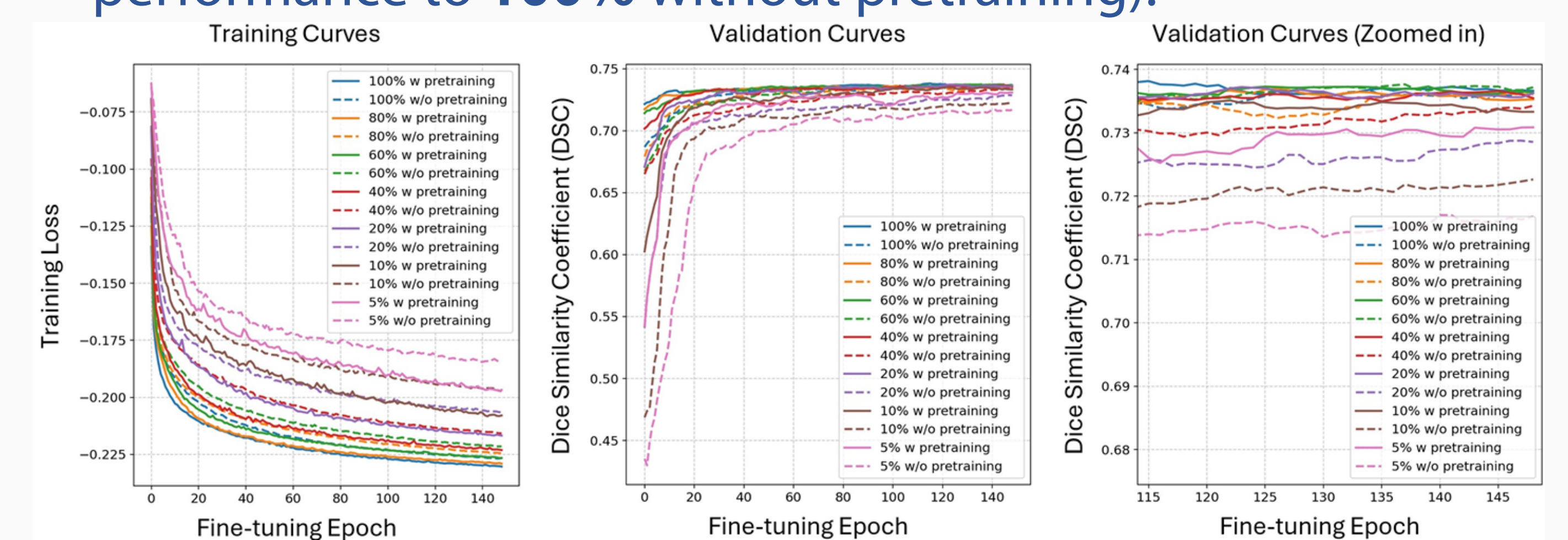
Pretrained models demonstrated **superior or equivalent performance** (*Dice score*:  $0.751 \pm 0.122$ ) compared to training-from-scratch ( $0.749 \pm 0.125$ ) and baseline methods, including SynthMorph ( $0.688 \pm 0.152$ ), deedsBCV ( $0.740 \pm 0.127$ ), and ConvexAdam ( $0.749 \pm 0.126$ ).

### Efficiency and Data Reduction:

- Achieved accuracy on par with pretraining using in-domain data.



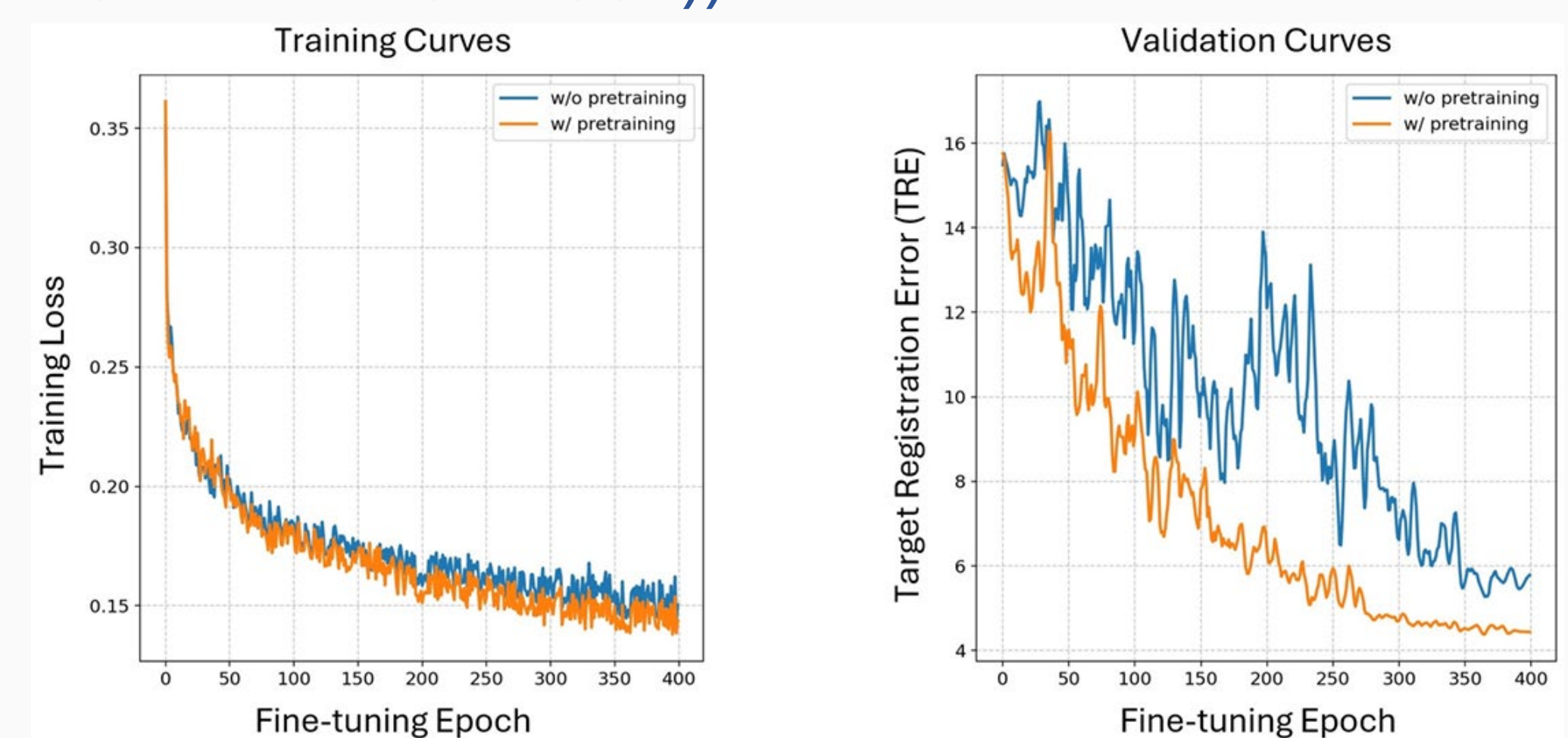
- Achieved competitive accuracy using substantially less labeled data (**10%** of training data achieved comparable performance to **100%** without pretraining).



- Reduced training times (encoder-only ~0.012 min/pair vs. full model ~0.022 min/pair).

### Generalizability to Other Domains:

Demonstrated applicability to limited-data lung registration tasks (TRE significantly improved from not using pretraining ( $2.753 \pm 2.029 \rightarrow 2.116 \pm 1.662$ )).



## Reference

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- Chen, Junyu, et al. MedIA 82 (2022): 102615.
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