

High resolution neural connectivity from incomplete tracing data using nonnegative spline regression

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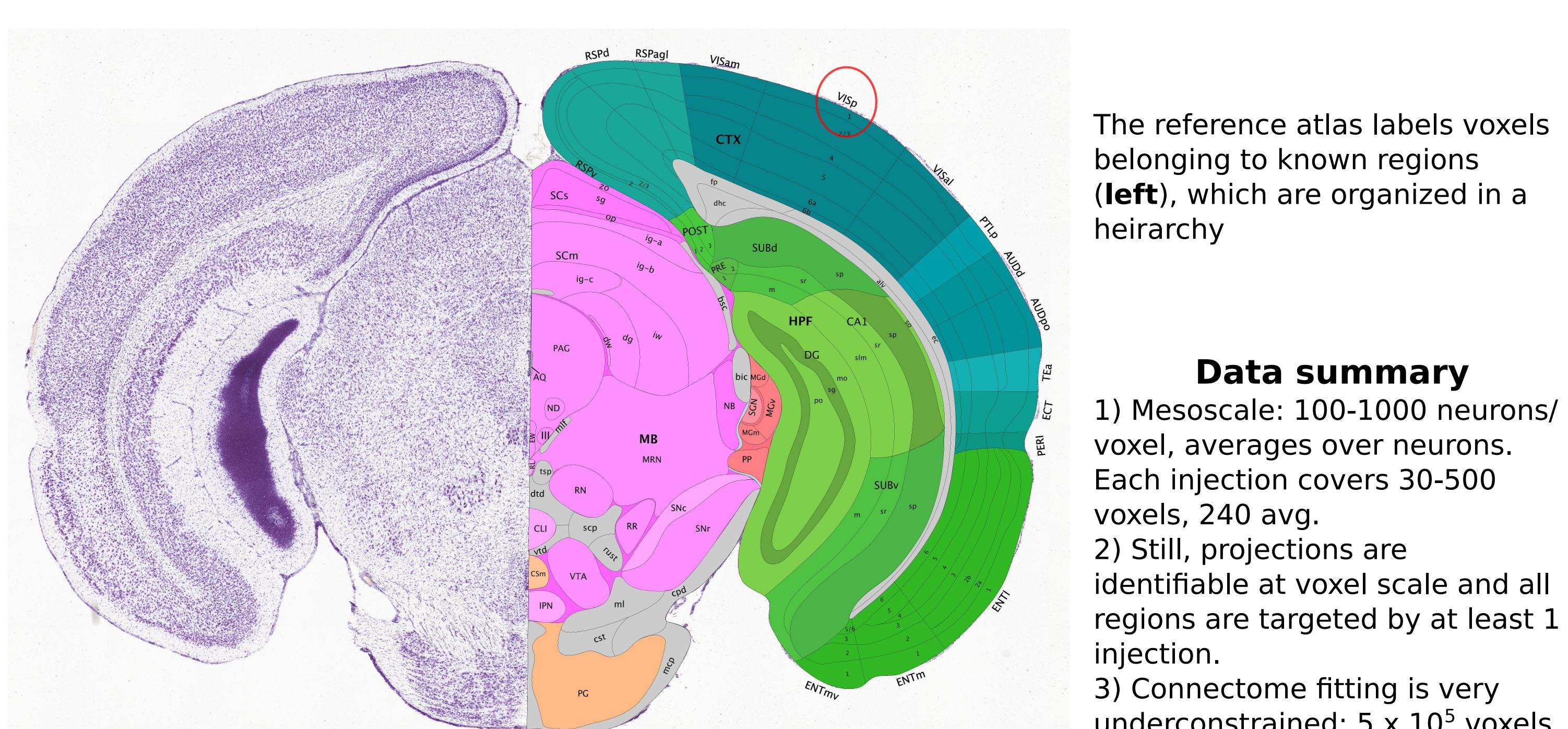
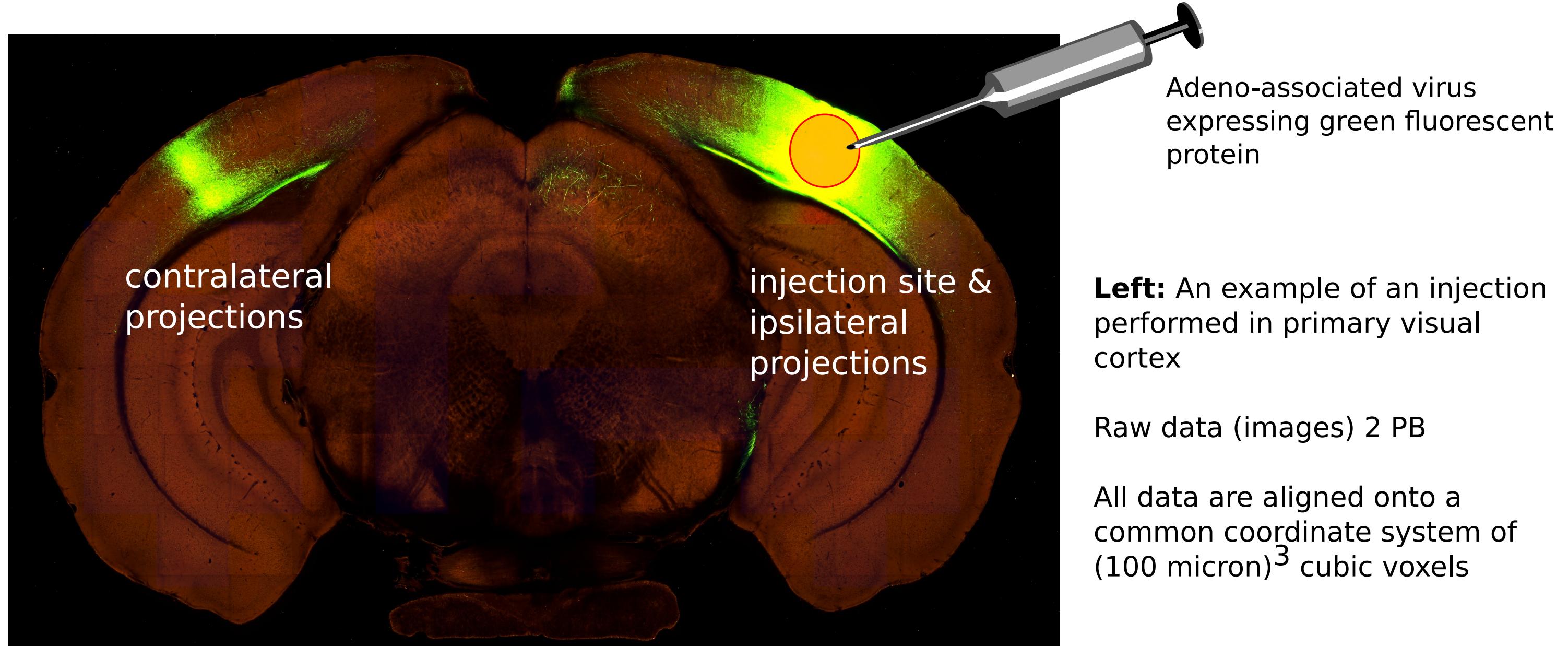
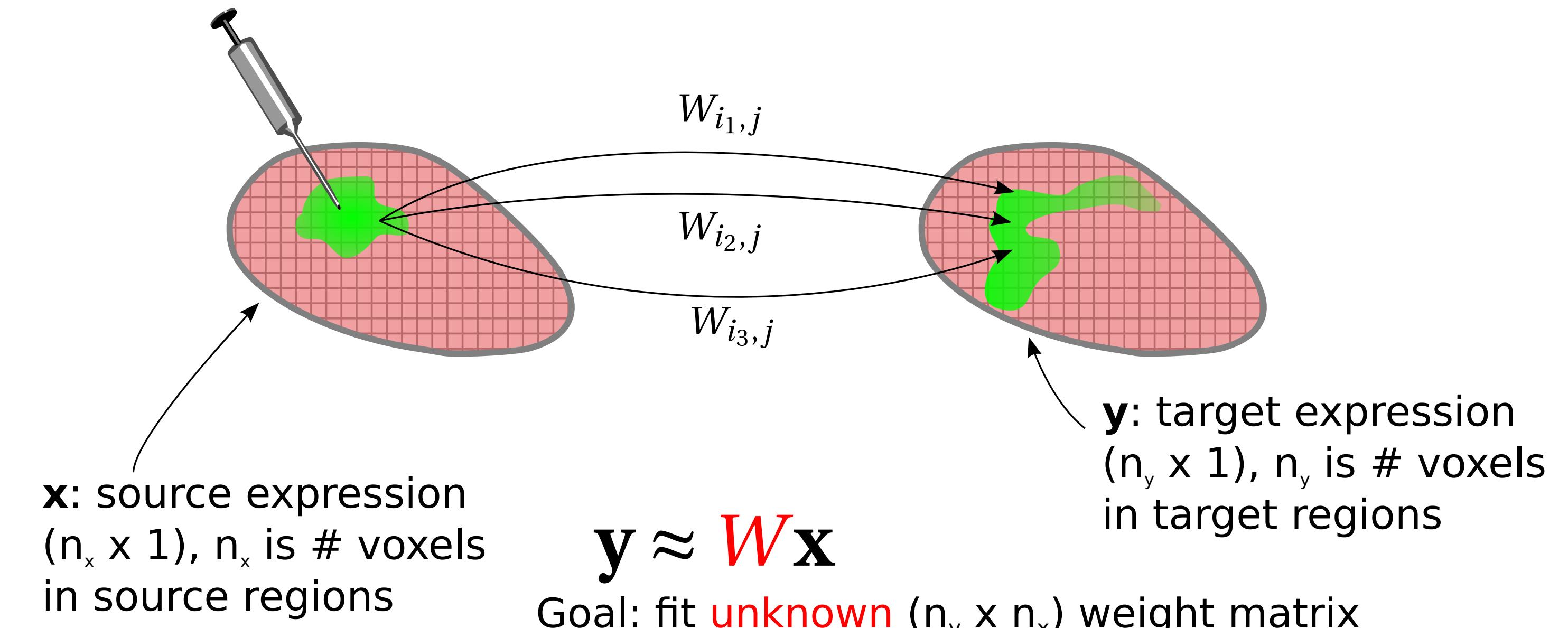
Code, movies, and more!
github.com/kharris/high-res-connectivity-nips-2016

Motivation

Scientific: Understand interplay of brain **network structure** and **information representation** (coding). Examine functional correlations such as spatial maps in relation to structural connectivity.

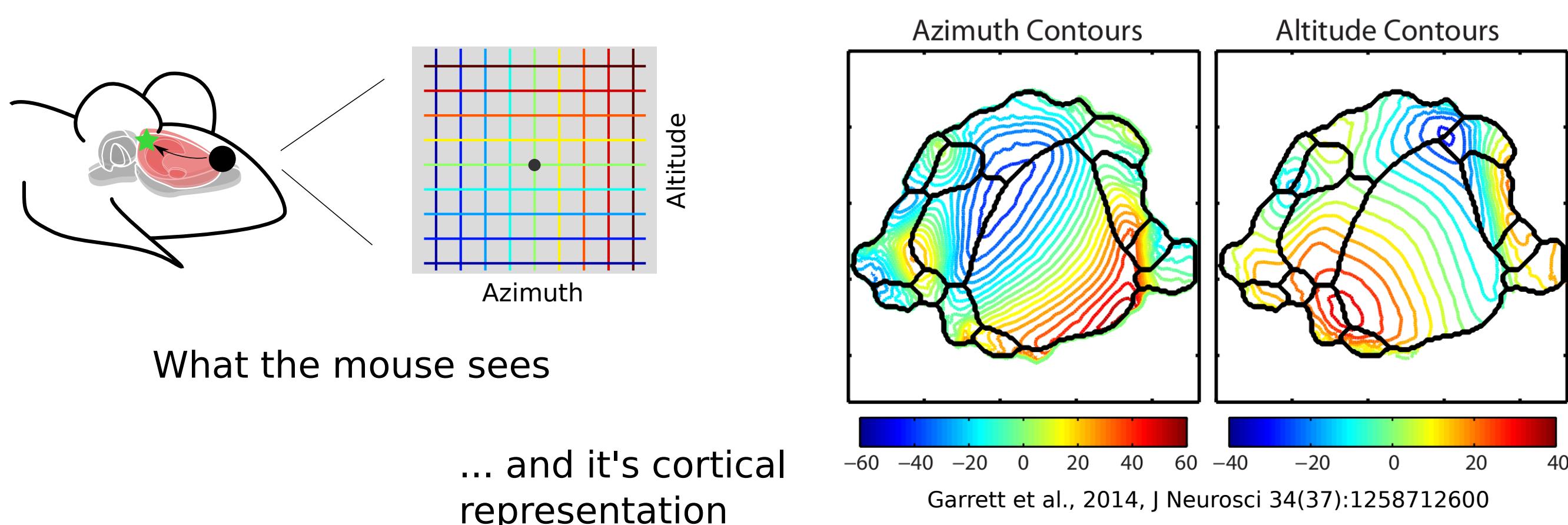
Mathematical: Develop tractable methods for analyzing high-dimensional structural connectivity data from next-generation experiments.

Tracing experiments



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Voxel model strategy: assume smoothness

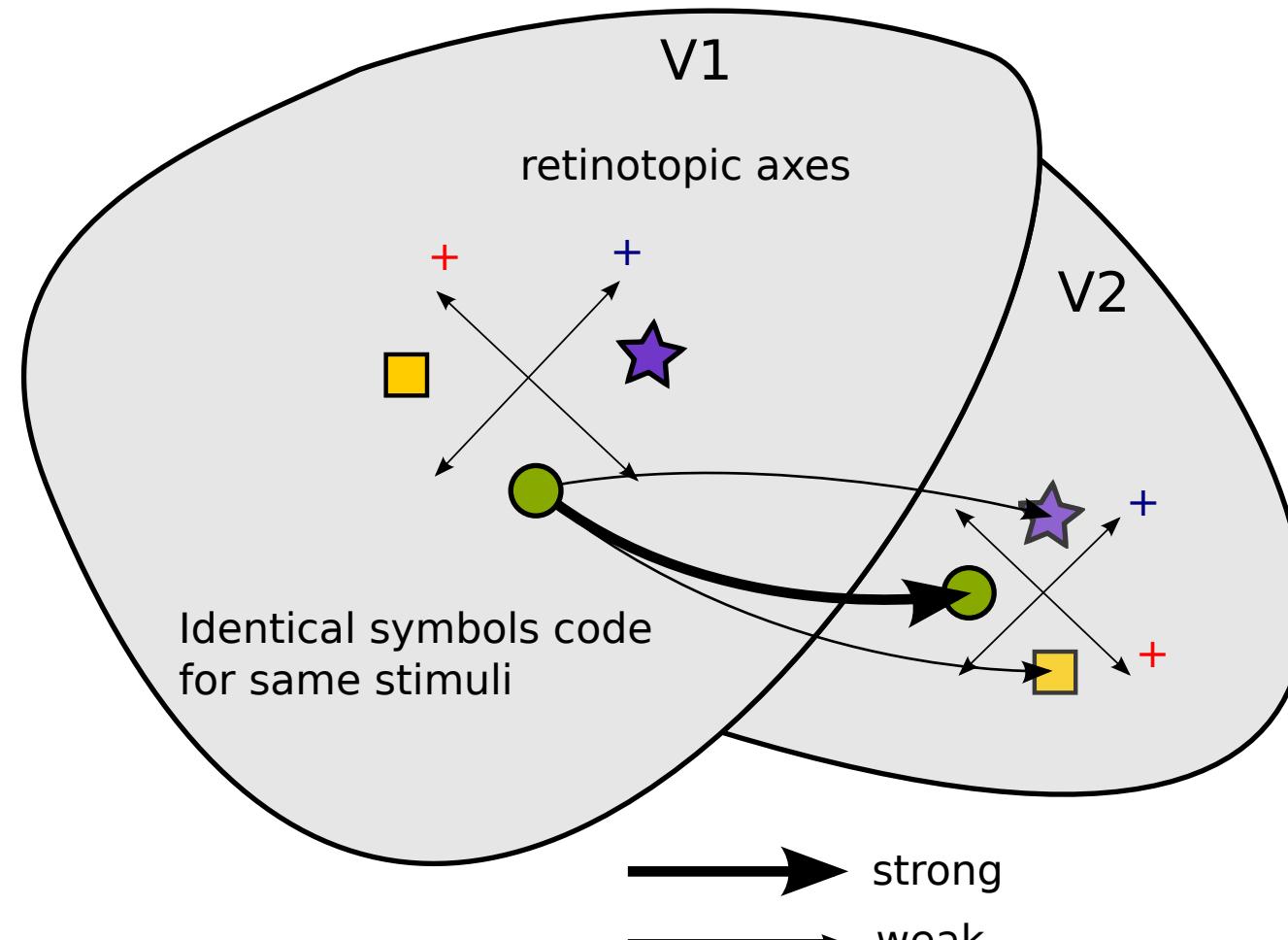


Retinotopy (map representation of visual field) in primary visual cortex is maintained from V1 into deeper areas analogous to V2, etc.

Assumptions:

- like connects strongest to like
- connection strength decreases as similarity decreases
- retinotopy (hence similarity) is smooth

Taken together, suggests connections vary smoothly in space



Smoothness regularized model

Find the voxel-resolution connection matrix W that balances goodness of fit and smoothness:

$$W^* = \arg \min_{W \succeq 0} \|P_\Omega(WX - Y)\|_F^2 + \lambda \frac{n_{\text{inj}}}{n_x} \|L_y W + WL_x^T\|_F^2$$

Goodness of fit (loss) term Smoothness (regularization) term

Data matrices:

$$Y = [y_1, \dots, y_{n_{\text{inj}}}]$$

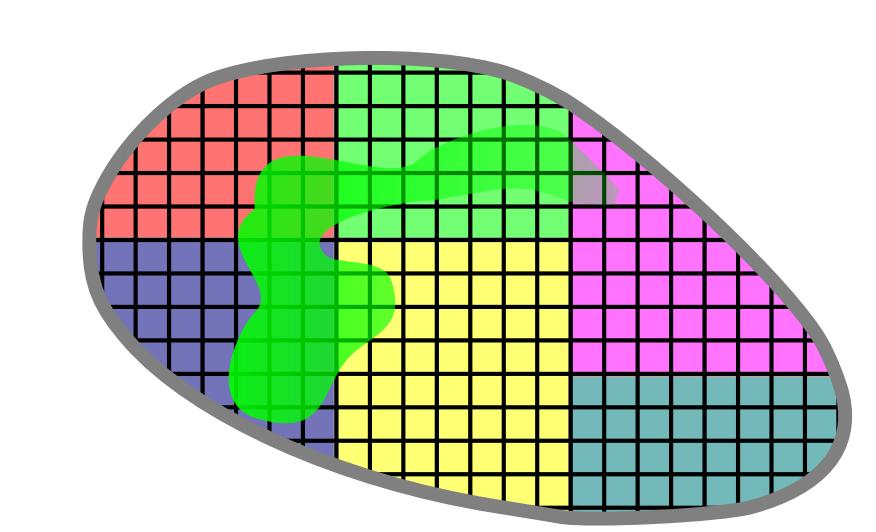
$$X = [x_1, \dots, x_{n_{\text{inj}}}]$$

P_Ω : Loss is summed only over voxels outside injection site, as in "matrix completion"

L_x , L_y : finite difference Laplacian matrices. Regularization is analogous to so-called "thin-plate splines" radial basis functions for regression or interpolation

Previous work: regional model

Oh et al., 2014, Nature 508(7495):207-214



Fit the weight matrix $W^{(r)}$ via non-negative least squares

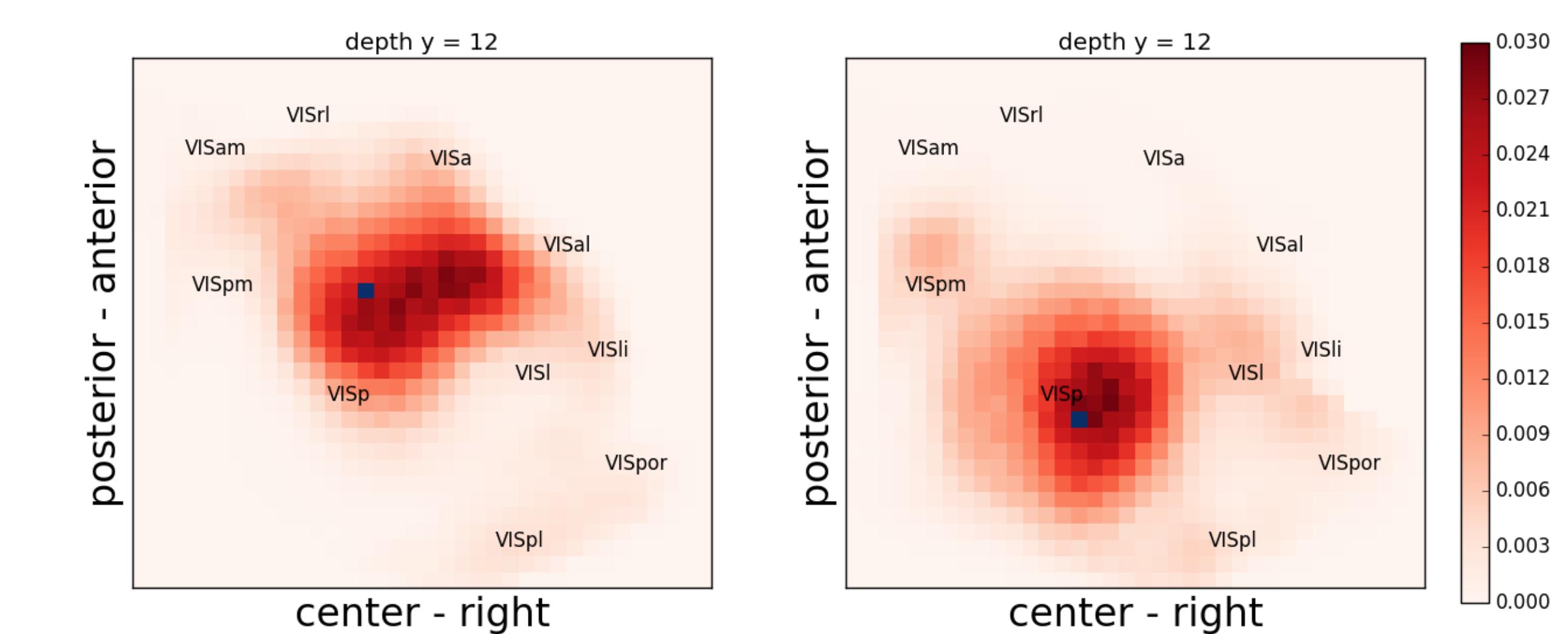
$$\min_W \|Y^{(r)} - W^{(r)} X^{(r)}\|_F^2$$

$$y_{i,j}^{(r)} = \int_{\text{region } i} \text{target signal of experiment } j$$

$$x_{i,j}^{(r)} = \int_{\text{region } i} \text{source signal of experiment } j$$

This is the same as choosing a voxel scale W where W_{ij} is constrained to be constant for all voxels i in region A and j in region B, for all regions A and B

Voxel approach begins to reveal spatial connectivity maps



Spatial connectivities are more predictive in cross-validation

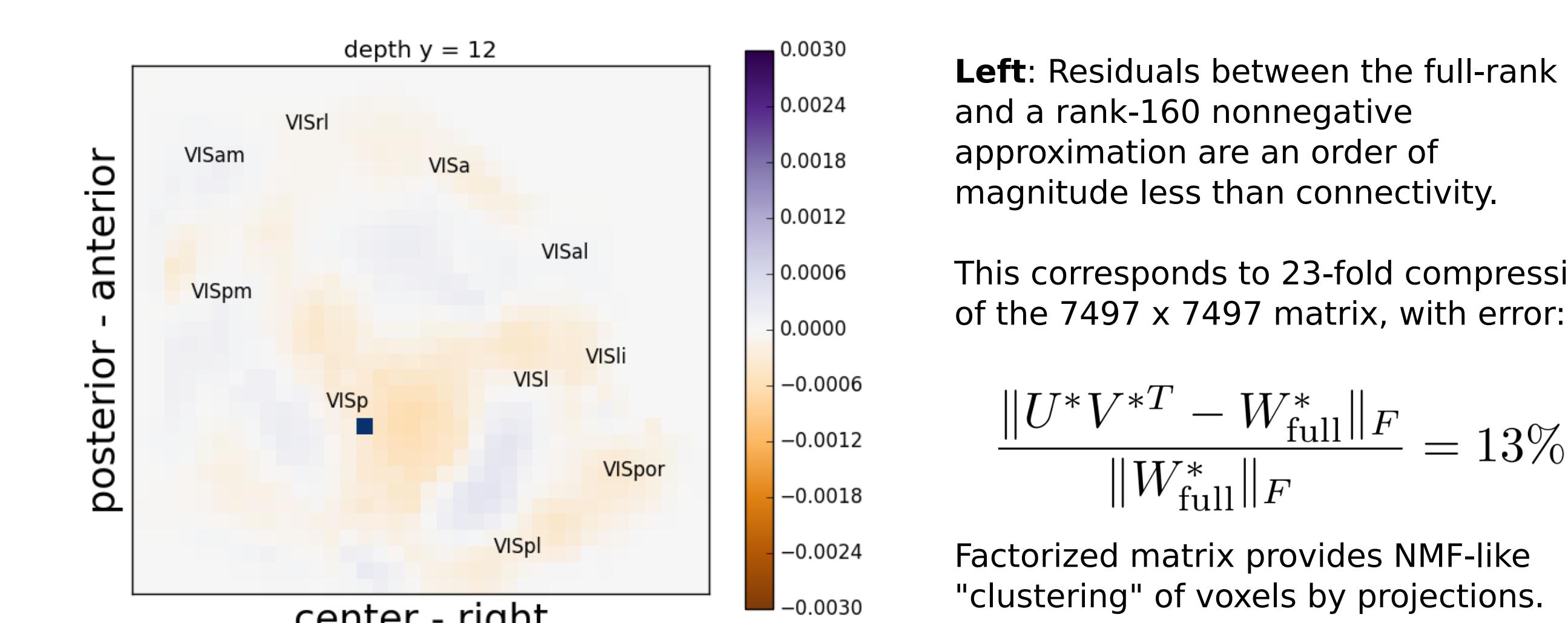
Model	Voxel MSE _{rel}	Regional MSE _{rel}
Regional	107% (70%)	48% (6.8%)
Voxel	33% (10%)	16% (2.3%)

$$\text{MSE}_{\text{rel}} = \frac{2\|P_\Omega(WX - Y)\|_F^2}{\|P_\Omega(WX)\|_F^2 + \|P_\Omega(Y)\|_F^2}$$

Low rank approximation enables inference that scales

Non-convex, low-rank version of previous spatial model:

$$(U^*, V^*) = \arg \min_{U, V \succeq 0} \|P_\Omega(UV^T X - Y)\|_F^2 + \lambda \frac{n_{\text{inj}}}{n_x} \|L_y UV^T + UV^T L_x^T\|_F^2$$



- Whole brain: number of voxels is 5×10^5
- Same 23-fold compressibility means rank 10^4
- This is still a problem in $O(10^9)$ unknowns
- Compresses W matrix from 1.9 TB to 75 GB

Challenges and future work

- Basis function representations: better than low rank?
- Compare Cre cell type-specific connectivity
- Compare spatial maps of retinotopy to connectivity
- Fit entire mouse brain, requires massive parallelization