

UNIVERSITY OF PATRAS - SCHOOL OF ENGINEERING
DEPARTMENT OF ELECTRICAL AND COMPUTER ENGINEERING



**ΠΑΝΕΠΙΣΤΗΜΙΟ
ΠΑΤΡΩΝ**
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DIVISION: SYSTEMS AND AUTOMATIC CONTROL

THESIS

of the student of the Department of Electrical and Computer Engineering of the School of
Engineering of the University of Patras

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Subject

**Robotic surgical tool manipulator - Recognition,
control and manipulation of laparoscopic tools**

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Thesis Number:

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ΠΙΣΤΟΠΟΙΗΣΗ

Πιστοποιείται ότι η διπλωματική εργασία με θέμα

Robotic surgical tool manipulator - Recognition, control and manipulation of laparoscopic tools

του φοιτητή του Τμήματος Ηλεκτρολόγων Μηχανικών και Τεχνολογίας Υπολογιστών

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Student: **Karadimos Alexios of Loukas**

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Associate Professor Dr. Evangelos Dermatas, University of Patras
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Thesis research period:

Abstract

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1 Introduction

1.1 Surgical robotics

1.1.1 Historical Overview of Surgical robotics

Surgical robotics is a field of Surgery where the surgeon operates on the patient via a computer, specialised equipment and robotic arms, to which the surgical tools needed for the operation are attached. According to surgical bibliography, robotics and laparoscopic procedures are used in general surgery, cardiothoracic surgeries, colon surgeries, gynecology, neurosurgery and orthopedics.

Robotic mechanisms were first introduced in Medicine, in 1987 with the first laparoscopic surgery of a cholecystectomy. Since then numerous laparoscopic operations have been performed and there has been a lot of improvements and innovations in this field. Such surgical operations are characterised as **minimally invasive**, because the surgical incisions made at the patient are very small and thus the probability of infection of the patient during or after the operation are very small, the hospitalization time is reduced (which means mean better and more efficient use of hospital resources) and the overall recovery of the patient is significantly faster and less painful.

However, traditional laparoscopic mechanisms have some downsides as well. First of all, the surgeon should operate in a mirrored-way, meaning that they should move at the opposite direction from what they saw at the screen (this effect is also known as the **fulcrum effect**), in order to reach the desired point of operation. Earlier laparoscopic tools had less degrees of freedom, which means less flexibility in motion control. Moreover these systems provided limited touch sensibility and feedback to the doctor they were very susceptible to the surgeon's micro movements and tremble.

The first application of robotics in Surgery appears in 1985, when Kwoh et al. [54] used a **PUMA 560**, a standard industrial robotic arm, to perform a neurosurgical biopsy, where the biopsy needle was inserted in the brain and guided with the help of Computed Tomography. This successful application was followed by the **PROBOT** surgical robot [42], which was developed at the Imperial College and used in a prostatectomy operation. Another example of an early surgery robot was the **ROBODOC** system [10] developed by Integrated Surgical Supplies in Sacramento California, which was the first to be used in orthopedics for a hip replacement surgery and was also the first to be approved by the FDA (Food & Drug Administration, organization responsible for medical devices, drugs etc.).



Figure 1: The PUMA 560 robotic arm, which was the first to be used in surgery robotics in 1985

Some other important surgery robots are listed below:

- **AESOP®Endoscope Positioner:** A voice controlled endoscopic system
- **HERMES®Control Center**

- **daVinci Surgical System®:** One of the most popular surgery robots and most used in hospitals. It is a master-slave system, which means that the operation commands are sent unidirectionally from the master console, which is controlled by the surgeon, and are executed by the robot. It also comes with a high definition 3D video feed and advanced manipulator system, one for each hand, called EndoWrist®. It is officially approved by the FDA for laparoscopic surgeries.

- **SOCRATES Robotic Telecollaboration System**

- **Raven-II [26]:** An open platform for collaborative research on surgical robotics.

- **Monarch™ Platform** by Auris Health Inc., an endoscopic system for robotic-assisted bronchoscopy



Figure 2: DaVinci Xi, ©2020 Intuitive Surgical, Inc. Patient Cart with the robotic arms that control the surgical tools



Figure 3: The MonarchTM Platform endoscopic system ¹

1.1.2 Surgical Robotics Procedure

The robotic surgery procedure starts with total anesthesia of the patient. Then the surgeon makes small incisions at the anatomical region of interest, where the procedure will take place. Through these small incisions special tubes, called trocars, are mounted, through which the laparoscopic tools are inserted. After the patient is prepared and after the patient cart, which carries the robotic arms, is successfully positioned and calibrated, the surgeon sits on a console, from where they control the robot via special sensitive joysticks. The surgeon has vision access (often in 3D) to the surgical site via a small endoscopic camera and the video is displayed on the console. In some cases, the surgeon gets force feedback from the joysticks via haptic mechanisms. Haptic force feedback is very important for the doctor in order to have a better sense of the anatomy and the surgical site, and it has gained a lot of interest in the research community.

¹<https://www.aurishealth.com/patients/robotic-bronchoscopy-patient-about-monarch-platform>



Figure 4: DaVinci Xi ©2020 Intuitive Surgical, Inc. Surgeon Console ²

1.1.3 Advantages & Disadvantages of Surgical robotics

Surgical robotics have a huge impact in Medicine and Healthcare in general. Some of the advantages are the following:

- **Minimally Invasive Procedures** which means
 - Smaller incisions
 - Less blood loss
 - Reduced risk of inpatient infection
 - Less pain
 - Faster patient recovery
- Increased **precision** and reduced human errors
 - Smooth and precise movements
 - Detection and correction of errors caused by hand tremble
- **No fulcrum effect** and intuitive manipulation of surgical tools
- **Haptic feedback.** This technology uses small mechanical forces and vibrations to give the user the sense of touch or force. Force feedback gives the ability to the surgeon to understand the mechanical properties of the tissue they operate on, such as resistance and elasticity, and thus distinguish between healthy from unhealthy tissue
- **Teleoperation** (currently in the same room only): the surgeon operates while they sit on a special **ergonomic** console, which makes the long procedures more comfortable and efficient.

²<https://www.intuitive.com/en-us/about-us/press/press-resources>

1.2 Problem statement

The goal of this thesis is to design the kinematic models and algorithms necessary for a robotic arm to detect, pick and manipulate a laparoscopic surgical tool. To achieve these goals the robotic arm must successfully do the following:

- Use computer vision to detect the scene and laparoscopic tools and with the help of stereoscopic vision, calculate the position and orientation of the center of mass of each tool, with respect to the universal reference frame
- Calculate the contact points on the tool, on which the fingers of the gripper will be placed, so that there is a firm grasp (force closure)
- Calculate the path from the tools' table to the surgical site table
- Calculate the trajectory that needs to be executed when the tool is inserted in the trocar. This is a special type of trajectory, because the motion is constrained and is known in the bibliography as a **Remote Center of Motion** (RCM) control. The constraint is that, at each time one point of the inserted tool must coincide with the RCM point (this point will also be referenced in this thesis as the center of the trocar, or the fulcrum reference frame point).

1.3 Bibliography Overview

1.4 Methodology & Approach

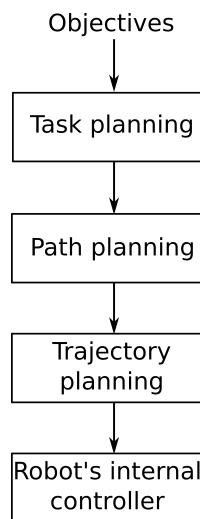


Figure 5: Motion planning pipeline

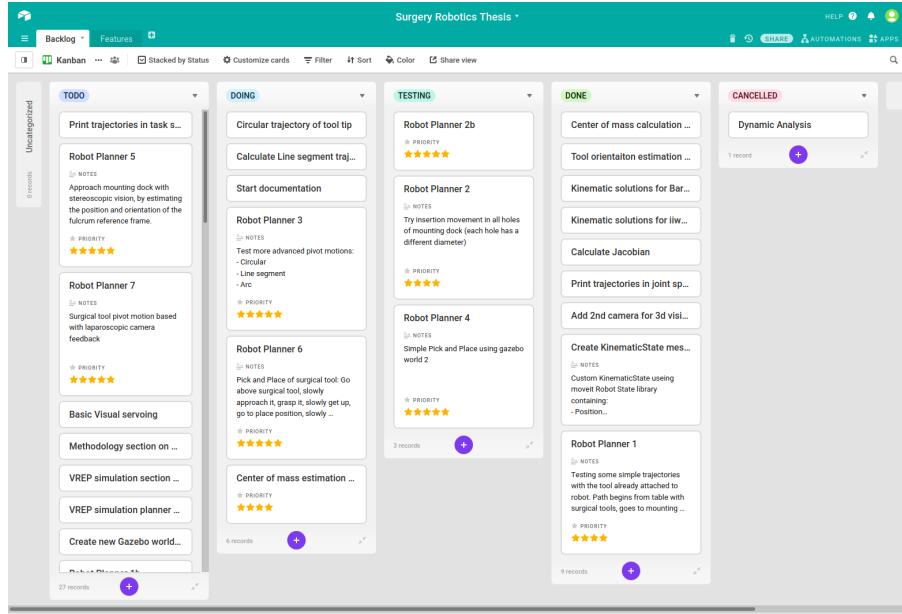


Figure 6: Kanban view of backlog tasks to organize all features, requirements and tasks needed to complete this thesis. The tool used to keep track of all tasks is Airtable

2 Robotic arm Kinematic Analysis

2.1 Robotic arm, DH parameters & Forward Kinematics

The Forward Kinematics problem seeks to specify the way in which the robot's links are connected together. In other words, we want to specify the transformations between every pair of consecutive robot links. It is known that the forward kinematics of a robot can be calculated given only four parameters for each link. These parameters are known in robotics as the **Denavit-Hartenberg** (DH) parameters. Two of these parameters describe the link itself and the other two describe the link's relation to the neighboring link.

- The **length** L_i of the i -th link is equal to the distance between the axes z_i and z_{i+1}
- The **twist angle** α_i of the i -th link, is the angle between the axes z_i and z_{i+1}
- The **rotation angle** θ_i of the link $\{i\}$ with respect to the $\{i - 1\}$ link, is the angle between the axes x_{i-1} and x_i
- The **distance** d_i of the link $\{i\}$ with respect to the $\{i - 1\}$ link, is the distance between the axes x_{i-1} and x_i

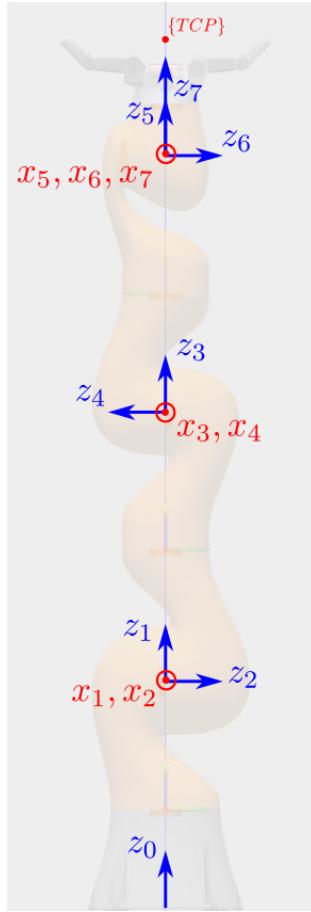


Figure 7: Joint reference frames of the KUKA iiwa14 robot

i	θ_i (rad)	L_{i-1} (m)	d_i (m)	α_{i-1} (rad)
1	θ_1	0	0.36	0
2	θ_2	0	0	$-\pi/2$
3	θ_3	0	0.36	$\pi/2$
4	θ_4	0	0	$\pi/2$
5	θ_5	0	0.4	$-\pi/2$
6	θ_6	0	0	$-\pi/2$
7	θ_7	0	0	$\pi/2$

Using the DH parameters of the above table, one can calculate the transformation matrix between two consecutive links, and is calculated as the following

$${}^{i-1}T_i = \begin{bmatrix} c\theta_i & -s\theta_i & 0 & L_{i-1} \\ s\theta_i c a_{i-1} & c\theta_i c a_{i-1} & -s a_{i-1} & -s a_{i-1} d_i \\ s\theta_i s a_{i-1} & c\theta_i s a_{i-1} & c a_{i-1} & c a_{i-1} d_i \\ 0 & 0 & 0 & 1 \end{bmatrix} \quad (2.1.1)$$

When all the neighboring transformations are calculated, then one can calculate the total transformation 0T_N , which represents the position and the orientation of the local coordinate system of the end-effector with respect to the global coordinate system of the robot's base. The orientation is the upper-left 3x3 matrix and the position is given by the fourth column of the matrix 0T_N .

$${}^0T_N = {}^0T_1 \cdot {}^1T_0 \cdots {}^{N-1}T_N \quad (2.1.2)$$

2.2 Inverse Kinematics

2.2.1 Decoupling Technique

In this section the inverse kinematics problem is solved for only the 6 out of the 7 total degrees of freedom. The third joint is not used in this analysis and its angle is set to zero $\theta_3 = 0$. The rest of the joints form a special kind of kinematic chain that can be solved using the decoupling technique. In this technique the Inverse kinematics problem is split to 2 separate subproblems, one for the position and one for the orientation of the end-effector. This technique can be applied in this case because the axes of the 3 last joints intersect at the same point and they form an Euler wrist.

To solve for the joints' angles, the transformation matrix 0T_7 of the end-effector with respect to the robot's base is required. Usually the transformation ${}^U T_{tcp}$ is known, which is the pose of Tool's center point (TCP) with respect to the Universal Coordinate Frame $\{U\}$ from which the required 0T_7 can be calculated

$${}^U T_{tcp} = {}^U T_0 \ {}^0 T_7 \ {}^7 T_{tcp} \quad (2.2.1)$$

$${}^0 T_7 = {}^U T_0^{-1} \ {}^U T_{tcp} \ {}^7 T_{tcp}^{-1} \quad (2.2.2)$$

$${}^0 T_7 = \begin{bmatrix} R_t & \mathbf{p}_t \\ 0 & 1 \end{bmatrix} \quad (2.2.3)$$

where ${}^U T_0$, ${}^7 T_{tcp}$ are translation transformations by a constant distance and R_t , \mathbf{p}_t are the target's orientation and position respectively.

$${}^0 \mathbf{p}_5 = {}^0 T_4 {}^4 \mathbf{p}_5 = \begin{bmatrix} p_x \\ p_y \\ p_z \end{bmatrix} \quad (2.2.4)$$

$$\theta_1 = \begin{cases} \text{atan2}(p_y, p_x) \\ \pi - \text{atan2}(p_y, p_x) \end{cases} \quad (2.2.5)$$

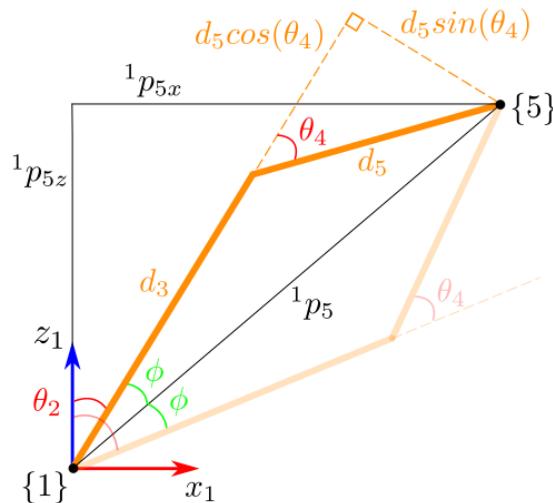


Figure 8: Calculation of angles θ_2, θ_4

$$\varphi = \arccos \left(\frac{d_3^2 + \|{}^1 p_5\|^2 - d_5^2}{2d_3 \|{}^1 p_5\|} \right) \quad (2.2.6)$$

$$\theta_2 = \text{atan2} \left(\sqrt{p_x^2 + p_y^2}, {}^1 p_{5z} \right) \pm \varphi \quad (2.2.7)$$

$$c_4 = \frac{\|{}^1 p_5\|^2 - d_3^2 - d_5^2}{2d_3 d_5}$$

$$\theta_4 = \text{atan2} \left(\pm \sqrt{1 - c_4^2}, c_4 \right) \quad (2.2.8)$$

Once $\theta_1, \theta_2, \theta_3, \theta_4$ are known, the orientation matrix of the wrist can be calculated as following

$$R_{target} = \begin{bmatrix} i_x & j_x & k_x \\ i_y & j_y & k_y \\ i_z & j_z & k_z \end{bmatrix}$$

$$\theta_6 = \text{atan2} \left(\pm \sqrt{1 - k_y^2}, k_y \right) \quad (2.2.9)$$

$$\theta_7 = \text{atan2} (-j_y, i_y)$$

$$\theta_5 = \text{atan2} (-k_z, k_x)$$

2.2.2 Workspace constraints & Singularity points

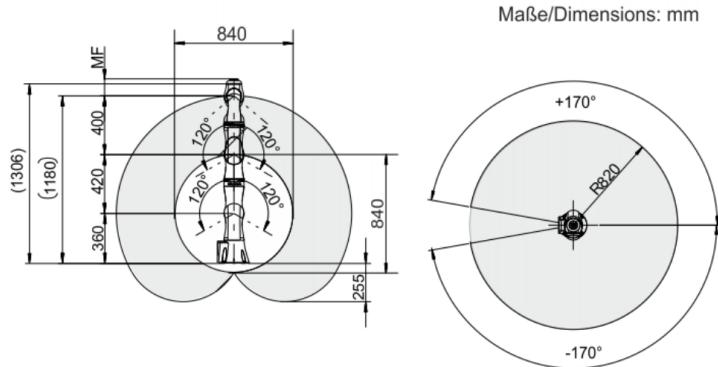


Figure 9: KUKA iiwa LBR14 workspace dimensions

Singularity points:

- When $p_x^2 + p_y^2 = 0$ then the end-effector lies on the z-axis and θ_1 is not defined
- When $\sin(\theta_6) = 0$ then the angles θ_5, θ_7 are not defined

2.2.3 Solutions for 7DoF numerically

Jacobian

$$J = J(\mathbf{q}) = [J_1, J_2, \dots, J_7] \in \mathbb{R}^{6 \times 7}$$

$$J_i = \begin{bmatrix} {}^0 \mathbf{z}_i \times ({}^0 \mathbf{p}_8 - {}^0 \mathbf{p}_i) \\ {}^0 \mathbf{z}_i \end{bmatrix} \quad (2.2.10)$$

$J(\mathbf{q})$ is non rectangular and thus non-invertible. Instead of the inverse of the Jacobian the pseudoinverse is calculated which by the equation

$$J^\dagger = J^\top (J J^\top)^{-1} \quad (2.2.11)$$

2.2.4 Comparison of Inverse Kinematics Techniques

3 Grasping

3.1 Gripper & Forward Kinematics

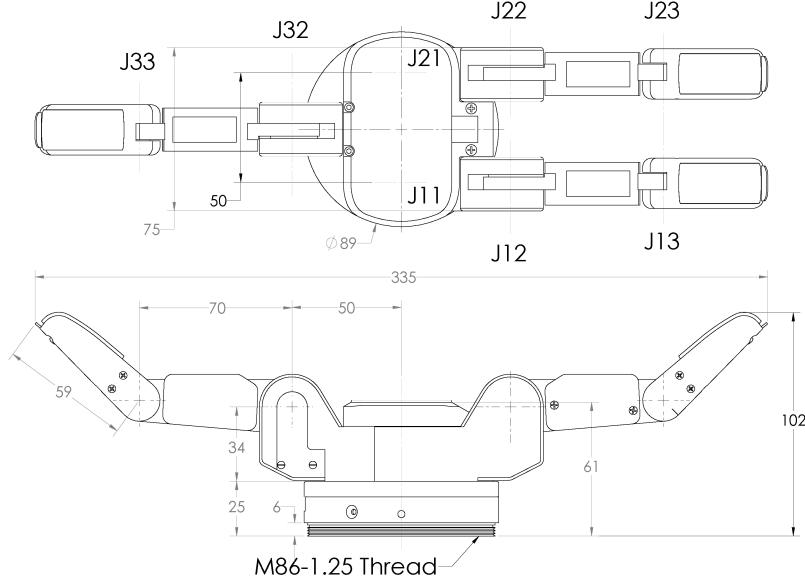


Figure 10: Barrett Hand gripper (model BH8-282) dimensions

3.2 Gripper Inverse Kinematics

The following Inverse Kinematics analysis refers to one finger of the Barrett Hand gripper, which has 3 revolute joints. Finger 3 has only 2 revolute joints for which the angle solutions are the same with the solutions of the last 2 joints of the other fingers. Let

$$\mathbf{p} = \begin{bmatrix} p_x \\ p_y \\ p_z \end{bmatrix}$$

be the position of the grasp point for one finger. The first angle can easily be calculated as

$$\varphi_1 = \text{atan2}(p_y, p_x) \quad (3.2.1)$$

Next, we calculate the third angle based on the law of cosines (see fig.)

$$\begin{aligned} \cos\left(\pi - \varphi_3 - \frac{\pi}{4}\right) &= \frac{L_2^2 + L_3^2 - p^2}{2L_2L_3} \\ \cos\left(\varphi_3 + \frac{\pi}{4}\right) &= \frac{p^2 - L_2^2 - L_3^2}{2L_2L_3} \\ \varphi_3 &= \text{atan2}\left[\pm\sqrt{1 - \left(\frac{p^2 - L_2^2 - L_3^2}{2L_2L_3}\right)^2}, \frac{p^2 - L_2^2 - L_3^2}{2L_2L_3}\right] - \frac{\pi}{4} \end{aligned} \quad (3.2.2)$$

In a more general case, the first argument of the *atan2* function in the expression of φ_3 could also be negative, but in this case this second solution is rejected, because due to mechanical constraints, this angle can't be negative. After having calculated φ_3 we can calculate φ_2

$$\begin{aligned} \tan(\psi + \varphi_2) &= \frac{p_z}{\sqrt{p_x^2 + p_y^2}} \\ \tan(\psi) &= \frac{L_3 \sin(\varphi_3 + \frac{\pi}{4})}{L_2 + L_3 \cos(\varphi_3 + \frac{\pi}{4})} \\ \varphi_2 &= \text{atan2}(p_z, \sqrt{p_x^2 + p_y^2}) - \text{atan2}\left[L_3 \sin\left(\varphi_3 + \frac{\pi}{4}\right), L_2 + L_3 \cos\left(\varphi_3 + \frac{\pi}{4}\right)\right] \end{aligned} \quad (3.2.3)$$

3.3 Force closure

The planar case, the spatial case & convex hull test.

3.4 Firm grasping algorithm & Force control

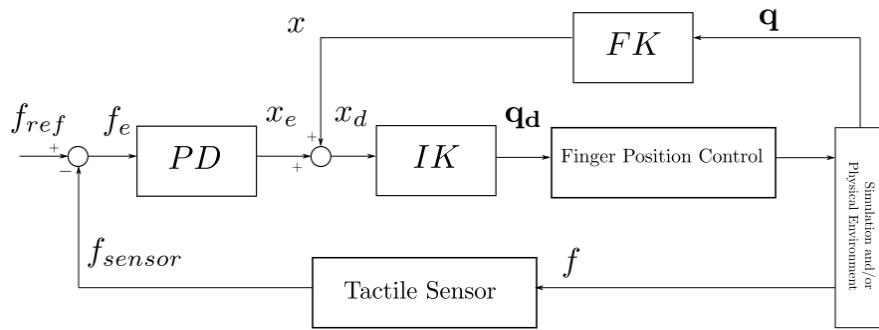


Figure 11: Force control on a Barrett Hand gripper finger

Listing 1: Example ROS message with collision/contact information between one finger of the gripper and one surgical tool

```

header:
  seq: 327978
  stamp:
    secs: 564
    nsecs: 468000000
  frame_id: "world"
states:
-
  info: "Debug: geom:surgical_tool4::surgical_tool_link::collision ..."
  collision1_name: "surgical_tool4::surgical_tool_link::collision"
  collision2_name: "robot::bh_finger_33_link::bh_finger_33_link_collision"
  wrenches:
  -
    force:
      x: -1.42463913929e-91
      y: 1.47711790023e-91
      z: -1.58225043603e-91
    torque:
      x: 5.44545932609e-93
      y: -3.73283810062e-93
      z: -8.38783555513e-93
  total_wrench:
    force:
      x: -1.42463913929e-91
  
```

```

y: 1.47711790023e-91
z: -1.58225043603e-91
torque:
  x: 5.44545932609e-93
  y: -3.73283810062e-93
  z: -8.38783555513e-93
contact_positions:
  -
    x: -0.00130886196029
    y: -0.587570558845
    z: 1.0584908858
contact_normals:
  -
    x: 0.041868681791
    y: -0.00620219851863
    z: -0.999103871586
depths: [4.625789111756262e-07]

```

4 Scene and object recognition with Computer Vision and Visual Servoing

At this section we explore ways to detect and recognize the surgical tools as well as other objects of the simulation scene. To reduce the complexity of this thesis and focus on the more important features of this thesis, we assume in the simulation that the surgical tools are blue and the mounting dock, where the tools will be placed, is green. These assumptions make the scene and object recognition much easier without the need of more advanced image processing and/or machine learning recognition algorithms.

Camera setup used in this thesis:

- 2 HD RGB cameras with resolution 1280×720
- near clipping plane: 0.02
- far clipping plane: 300
- horizontal FoV (field of view): 1.396
- update rate: 30fps

4.1 Laparoscopic tool detection

In order to detect the shape of the tool there are some standard steps that need to be executed. After having loaded the input image we convert it to grayscale, so that we can work on only one channel instead of 3 color channels and thus reduce the amount of calculations. Also for the purposes of extracting the shape of an object, the color doesn't have a very significant role in the algorithm. Next step is to remove the unwanted noise. In this thesis we only assume that the video frames have only Additive White Gaussian Noise (AWGN). To remove some of the noise we use a moving average filter (the filter is also known as a kernel), which is convoluted around the whole image. The filter that was used is the following 3-by-3 matrix

$$h = \frac{1}{9} \begin{bmatrix} 1 & 1 & 1 \\ 1 & 1 & 1 \\ 1 & 1 & 1 \end{bmatrix}$$

the output, filtered image is the result of the convolution of the image with the filter and is calculated as following

$$g(i, j) = \sum_{k,l} f(i + k, j + l)h(k, l) \quad (4.1.1)$$

where $g(\cdot, \cdot)$ is the output image and $f(\cdot, \cdot)$ is the input image.

After the noise is removed the image is getting binarized. To do that, we set a threshold, below which the pixels will be black and the rest will be white. This conversion to binary format, makes it easier to extract the boundaries of the black shapes, which will correspond to the boundaries of the objects of the initial image.

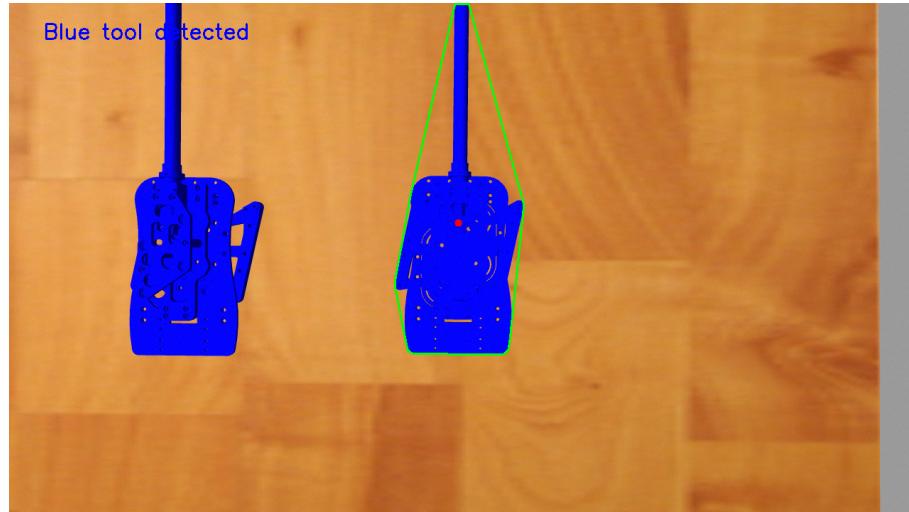


Figure 12: Simple tool detection in simulation based on color, using OpenCV. The green polygon is the convex hull, and the red point is the estimated center of mass

4.2 Stereoscopic vision

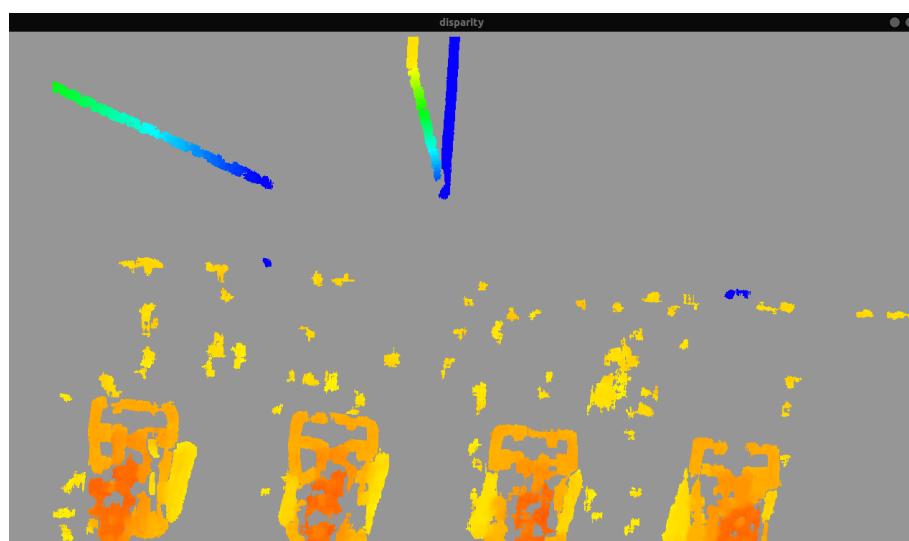


Figure 13: Disparity image calculated from the 2 cameras

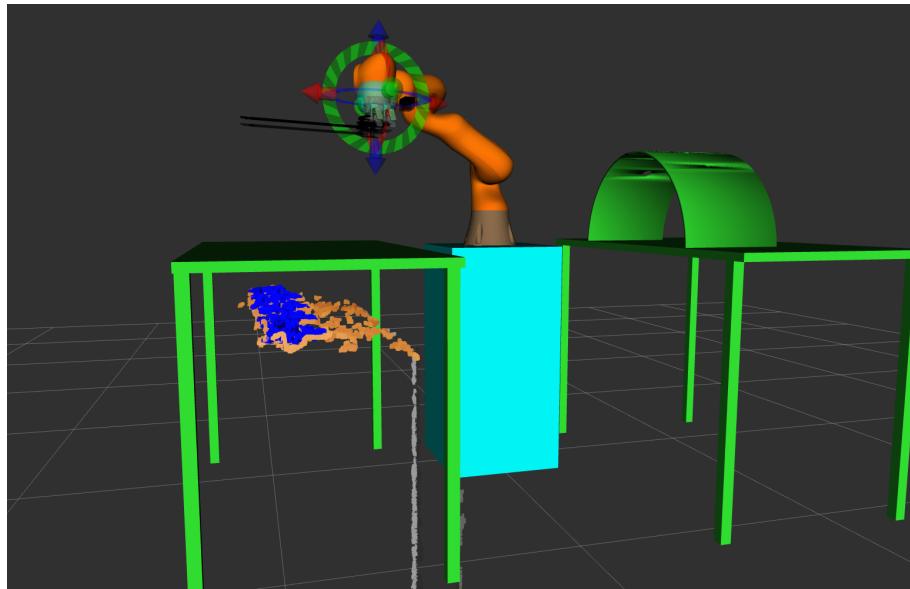


Figure 14: Point cloud of surgical tools, generated from the 2 cameras and visualized in RViz

4.3 Calculation of tool position and orientation

In order for the gripper to grasp correctly the laparoscopic tool, it is required to calculate the tool's position and orientation in the pixel space which must then be converted with respect to the robot's workspace. From all the pixels that have been classified as part of the laparoscopic tool, one can estimate the center of mass and two perpendicular vectors attached to that point that define the orientation. The center of mass is simply the average of the (x, y) coordinates of all the tool's pixels

$$(\bar{x}, \bar{y}) = \left(\frac{1}{N} \sum_{i=1}^N x_i, \frac{1}{N} \sum_{i=1}^N y_i \right) \quad (4.3.1)$$

The easiest way to calculate the center of mass is by calculating the average using the first moments of the contour points. However, since the contour is only using the boundary of the object and not its area, this method is not very accurate. To get a more accurate value for the center of mass, one must use the pixels that are inside the detected object's contour. The simplest way (but most expensive) to get the inside pixels of the tool is to loop over all the pixels and for each pixel check if it is inside the polygon (point inside polygon test). To make this method even faster, one can take a sample of the total pixels, for example check one in every 10 pixels in the x and y coordinates, which means reducing the time complexity to one tenth.

Taking this approach a step further in optimization, one can iterate not in all the video frame pixels but only those pixels that are inside the **Region of Interest** of the tool. The Region of Interest, also known as ROI, is a widely used structure in computer vision and is simply a bounding box (rectangle) that fits exactly (or is a bit bigger than) an object or part of the image frame that we want to study. Having already calculated the contour of the surgical tool and its convex hull we can easily calculate this bounding box. For this calculation we prefer to use the convex hull, because it often contains much less pixels than the contour. We iterate over all the pixels of the convex hull and we get the minimum and maximum x and y coordinates. The combination of these four values is the desired ROI. Since we now have access to the tool's ROI, we can iterate and sample the pixels inside it (and not all pixels as we did before) to get some of the pixels of the tool so that we can more accurately calculate its center of mass and orientation vectors.

The two orientation vectors are the eigenvectors of the covariance matrix of the above pixels. Let \mathbf{a}, \mathbf{b} be the orientation vectors, then \mathbf{a}, \mathbf{b} are solutions of the equation

$$C\mathbf{v} = \lambda\mathbf{v} \quad (4.3.2)$$

where C is the covariance matrix given by

$$C = \begin{bmatrix} \sigma(x, x) & \sigma(x, y) \\ \sigma(y, x) & \sigma(y, y) \end{bmatrix} \quad (4.3.3)$$

$$\sigma(x, y) = \frac{1}{n-1} \sum_{i=1}^N (x_i - \bar{x})(y_i - \bar{y}) \quad (4.3.4)$$

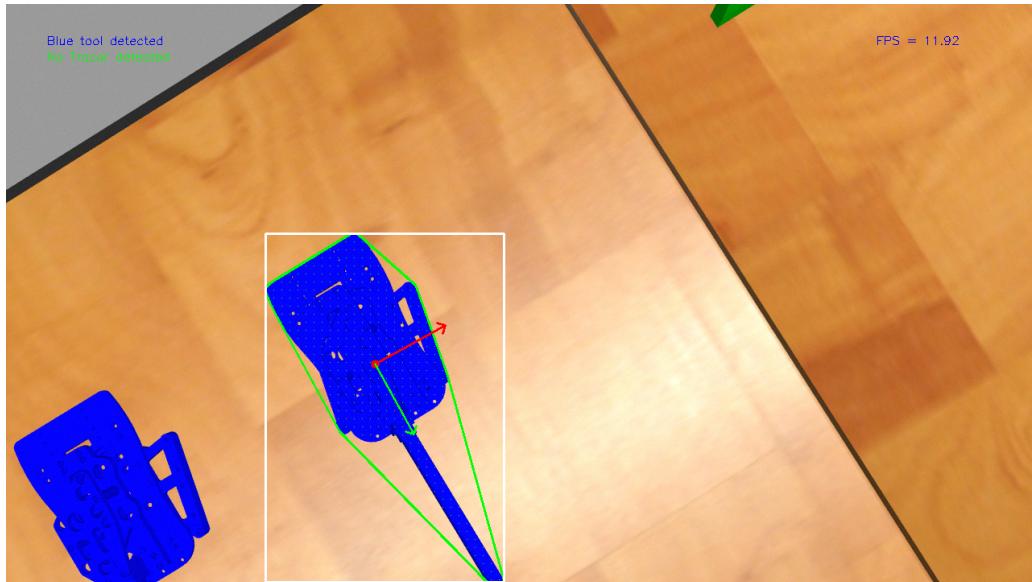


Figure 15: Estimation of tool's pose (position and orientation). The red dot is the center of mass and attached to that are the two orientation vectors of the tool. The green polygon is the convex hull of the tool and the white rectangle is it's ROI as calculated from the convex hull

4.4 Calculation of grasping points

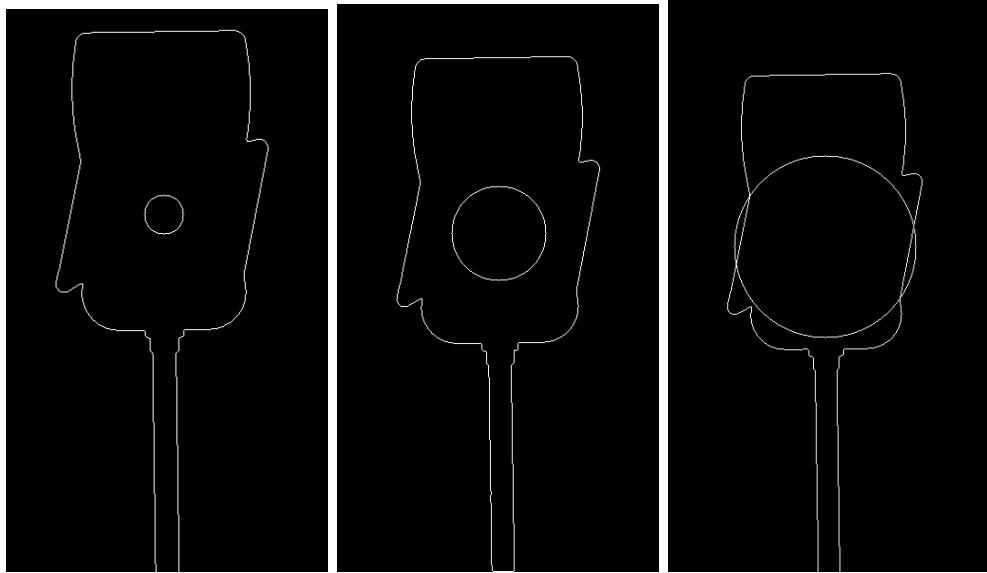


Figure 16: Finding candidate grasping points from the intersections of a growing circle and the contour of the detected surgical tool

The calculation of the candidate grasping points is a problem where we seek to find the points that lie on the contour of the detected object such that the gripper can make a good grasp of the object and preferably with force closure. The method that was implemented in this thesis for a simplistic calculation of these points is by using a **growing circle**. This circle is initiated with a small radius and has at all times its center at the center of mass of the detected tool. At each step of the method the radius is incremented by a fixed amount and then we check if this circle has any intersection with the contour of the detected tool. If no intersection is found the method proceeds with a new radius. The method is terminated when at least 3 intersections are found, and that's because the gripper that is used in this thesis has three fingers.

$$\mathbb{G} = \arg \max_{(x,y)} I_1(x,y) \odot I_2(x,y) \quad (4.4.1)$$

At the equation 4.4.1, the set of intersection points \mathbb{G} is calculated. Given one binary image $I_1(x,y)$ which contains the contour of the detected tool (all white pixels are the contour) and one second binary image $I_2(x,y)$ which contains the growing circle, then the set of intersection points are the (x,y) coordinates where the Hadamard product $I_1(x,y) \odot I_2(x,y)$ (element-wise product) of the two binary images is maximum (or equivalently has a value of 1).

It is often the case that for one intersection multiple pixels are returned from this method due to the "pixelated nature" of all curves. To filter all these pixels and get only one pixel for each intersection point we initialize a list of the final points with the first pixel found and then iterate over all of the other pixels. For each pixel we check if it has a Manhattan distance bigger than a threshold (e.g. 10) from the pixels that are already added in the list of the final pixels. If two pixels have a Manhattan distance bigger than a selected threshold then we consider them to be two different intersection points. The Manhattan distance of two points $\mathbf{p}_1 = (x_1, y_1)$, $\mathbf{p}_2 = (x_2, y_2)$ is given by

$$d_1(\mathbf{p}_1, \mathbf{p}_2) = |x_1 - x_2| + |y_1 - y_2| \quad (4.4.2)$$

4.5 Trocar detection & Estimation of fulcrum point

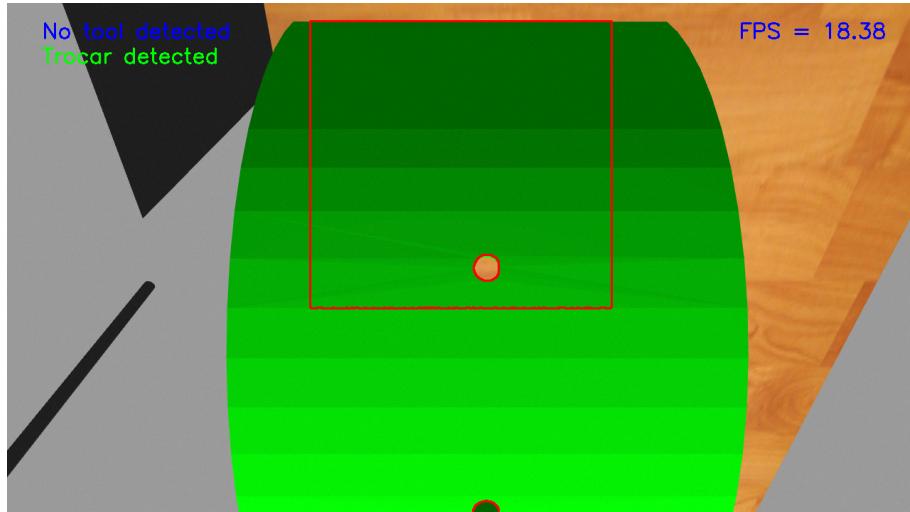


Figure 17: Simple trocar detection in simulation based on color, using OpenCV. In simulation, the trocar is simply considered to be a small cylindrical hole and it's center is the fulcrum point

4.6 Visual Servoing

At this chapter we briefly investigate how visual servoing can be applied in surgery robotics. **Visual Servoing** is the use of visual information to guide and control a robot. The main task of visual servoing is to control the end-effector's pose using features extracted from visual information. The features that are usually extracted from cameras are the position and orientation of the detected object, the distance of the object from the camera (using stereoscopic vision, photogrammetry or other techniques), the size and the shape of the object. The visual servoing can be executed either in the robot's space using position-based servoing or in the camera's space (also known as "pixel space") by using the image-based technique.

4.6.1 Position based servoing

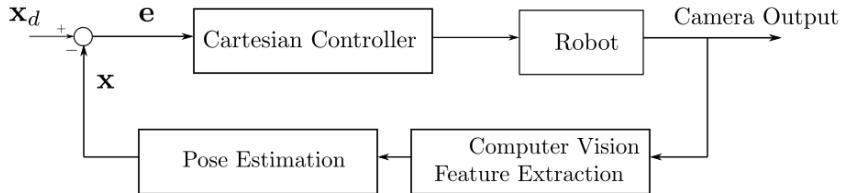


Figure 18: Position based visual servoing closed loop control

- **Photogrammetric technique**
- **Stereoscopic vision:** This methodology uses two separate views of the scene as taken from two viewports (from two cameras) and calculates the depth of various objects and areas using information from both views. For more details about stereoscopic vision see chapter 4.2
- **Extracting depth from motion** This methodology is very similar to stereoscopic vision and is also known as *monocular* or *motion stereo*. The difference is that instead of using two views from two distinct cameras this methodology uses two views from the same camera but from different points in time. A very important assumption for this methodology is to assume that two consecutive views from the video frame do not change significantly, so that some feature points can be matched in both views in order to calculate the depth information. This methodology is cheaper in terms of hardware but it fails to extract depth informations in cases where the robot is completely still.
- **Servoing using 3D sensors**

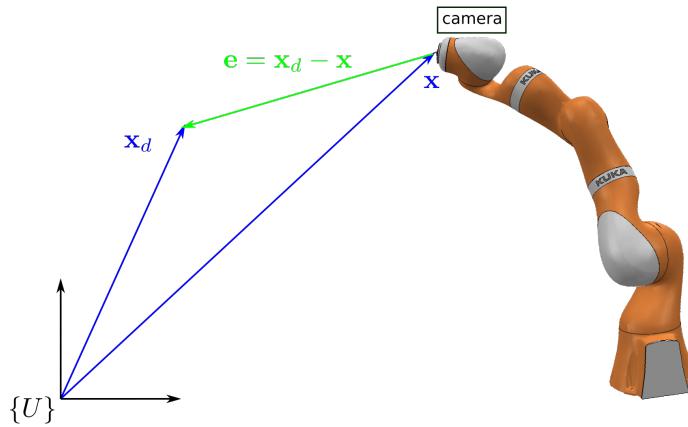


Figure 19: Position based visual servoing using depth from motion, stereo vision or 3D sensors, from which the desired position \mathbf{x}_d is calculated and used to drive the robot.

4.6.2 Image based servoing

Image based servoing is a methodology for controlling a robot by directly using features extracted from the image as well as positions on the image plane. The goal of this methodology is to drive the robot in such a way so that the video frame is changed from an initial view to a final, desired view (see figure 20 left and right frames). The commands that are sent to the robot from this methodology are defined in image space and not in the robot's task space. Moreover the distances calculated in image space are not directly related to distances in task space.



Figure 20: Image based visual servoing. The robot arm is controlled using the information gained from the video frames. The frames are 2Dimensional and thus the detected objects can have only 3 degrees of freedom which means we can mainly control 3 independent variables, here the x, y, θ variables. The left image is the initial frame and the right image is the frame where the object is at the target pose.

The image based visual servoing control system as depicted in figure 21 consists of the **Image Controller**, the **Plant** (robot) and the **feedback term**. The Image controller is a simple **PD Controller** (PID can also be used, but in servo systems PD is more common) which outputs commands to be executed in the plant. These commands are not to be confused with the robot's internal controller commands. These commands are to be used to control the robot in task space, whereas the internal controller drives each joint to the desired angle. The feedback used to calculate the error for the controller, uses the camera's output and based on that it calculates the vector from the detected tool's center of mass to the center of the image frame (feature extraction).

$$\mathbf{x}[(k+1)T] = \mathbf{x}[kT] + \mathbf{u}[kT] \quad (4.6.1)$$

where $\mathbf{x}[kT] = [x, y, z, \theta, \varphi, \psi]^\top$ and the discrete PID control law is given by equation 4.6.2

$$\mathbf{u}[kT] = K_p \left[\mathbf{e}[kT] + \frac{T}{T_i} \sum_{i=0}^{k-1} \mathbf{e}[iT] + \frac{T_d}{T} (\mathbf{e}[kT] - \mathbf{e}[(k-1)T]) \right] \quad (4.6.2)$$

where $\mathbf{e}[kT] = [e_x, e_y, e_z, e_\theta, e_\varphi, e_\psi]^\top$.

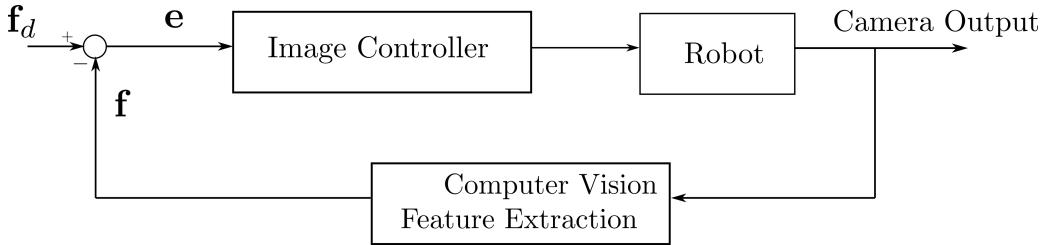


Figure 21: Image based visual servoing closed loop control

5 Path Planning - Laparoscopic tool manipulation

Path Planning is a geometric problem, where it is desired to find a path from a starting point to a goal point and also satisfying a set of constraints, such as: restricting the solutions inside the robot's configuration space, avoiding obstacles in the task space, avoiding singularity points and respecting the robot's joint limits.

The biggest challenge in manipulating a laparoscopic tool with a robot is overcoming the **fulcrum effect** problem. This is also one of the reasons that robotic assisted surgery replaced the traditional laparoscopic procedures. The fulcrum effect means that the surgeon's hand motions are inverted and scaled with respect to the Remote Center of Motion point, which lies approximately on the center of the incision. Apart from the scaling and inversion, laparoscopic procedures add an additional motion constraint that demands at each time one point of the laparoscopic tool to coincide with the RCM point.

5.1 Tool pose

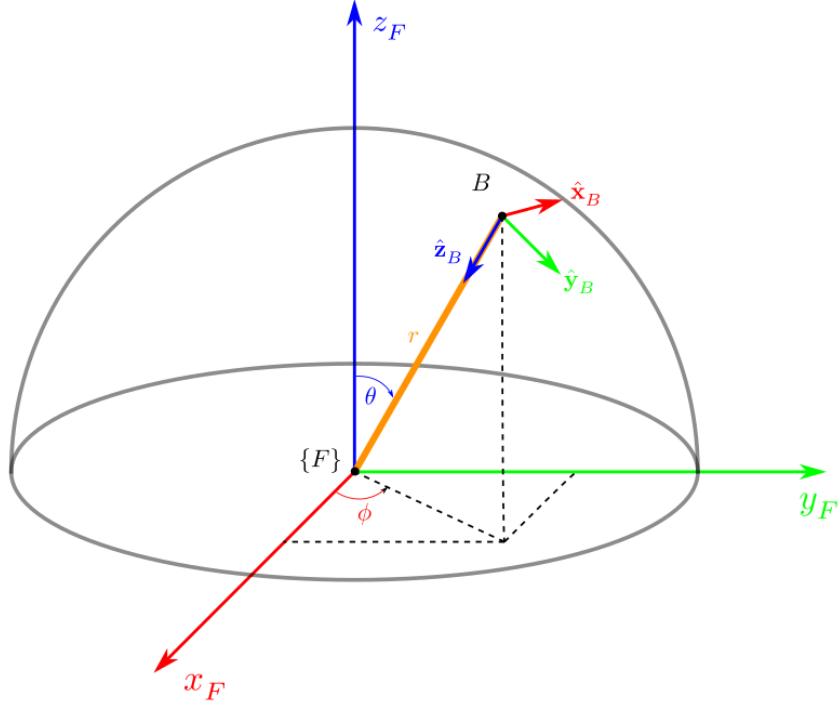


Figure 22: Tool pose at target point B calculated with respect to Fulcrum's reference frame $\{F\}$

The laparoscopic tool pose is given by the position and orientation vectors at target point B with respect to the coordinate frame $\{F\}$. The pose is given by the following transformation matrix

$${}^F T_B = \begin{bmatrix} {}^F R_B & {}^F \mathbf{p}_B \\ \mathbf{0} & 1 \end{bmatrix} \quad \text{where } {}^F R_B = [\hat{\mathbf{x}}_B \quad \hat{\mathbf{y}}_B \quad \hat{\mathbf{z}}_B]$$

$$\hat{\mathbf{x}}_B = \hat{\theta} = \cos(\theta)\cos(\varphi)\hat{\mathbf{x}}_F + \cos(\theta)\sin(\varphi)\hat{\mathbf{y}}_F - \sin(\theta)\hat{\mathbf{z}}_F = \begin{bmatrix} \cos(\theta)\cos(\varphi) \\ \cos(\theta)\sin(\varphi) \\ -\sin(\theta) \end{bmatrix} \quad (5.1.1)$$

$$\hat{\mathbf{y}}_B = \hat{\varphi} = -\sin(\varphi)\hat{\mathbf{x}}_F + \cos(\varphi)\hat{\mathbf{y}}_F = \begin{bmatrix} -\sin(\varphi) \\ \cos(\varphi) \\ 0 \end{bmatrix} \quad (5.1.2)$$

$$\hat{\mathbf{z}}_B = -\hat{\mathbf{r}} = -(\sin(\theta)\cos(\varphi)\hat{\mathbf{x}}_F + \sin(\theta)\sin(\varphi)\hat{\mathbf{y}}_F + \cos(\theta)\hat{\mathbf{z}}_F) = \begin{bmatrix} -\sin(\theta)\cos(\varphi) \\ -\sin(\theta)\sin(\varphi) \\ -\cos(\theta) \end{bmatrix} \quad (5.1.3)$$

The position of the point B is given in spherical coordinates by:

- $r = \rho$: outside penetration of laparoscopic tool
- $\theta = \beta$: altitude angle
- $\varphi = \alpha$: orientation angle

thus the position with respect to the coordinate frame $\{F\}$ is given by

$${}^F \mathbf{p}_B = \begin{bmatrix} \rho \sin(\beta) \cos(\alpha) \\ \rho \sin(\beta) \sin(\alpha) \\ \rho \cos(\beta) \end{bmatrix} = \rho \hat{\mathbf{r}} \quad (5.1.4)$$

The above goal point must be the same as the *TCP* point of the robot's end-effector. This means, that this pose must be converted with respect to the robot's reference frames.

$$\begin{aligned} {}^U T_{TCP} &= {}^U T_B \\ {}^U T_0 {}^0 T_7 {}^7 T_{TCP} &= {}^U T_F {}^F T_B \\ {}^0 T_7 &= {}^U T_0^{-1} {}^U T_F {}^F T_B {}^7 T_{TCP}^{-1} \end{aligned} \quad (5.1.5)$$

5.2 Pivoting motion with respect to Fulcrum Point

On this section, some basic pivoting trajectories around the fulcrum point, are presented. In all of the following three example pivoting motions, we have made the assumption that the position and orientation of the *F* reference frame is precisely known, which is however not applicable in real-life scenarios ()

5.2.1 Circular path of tool tip

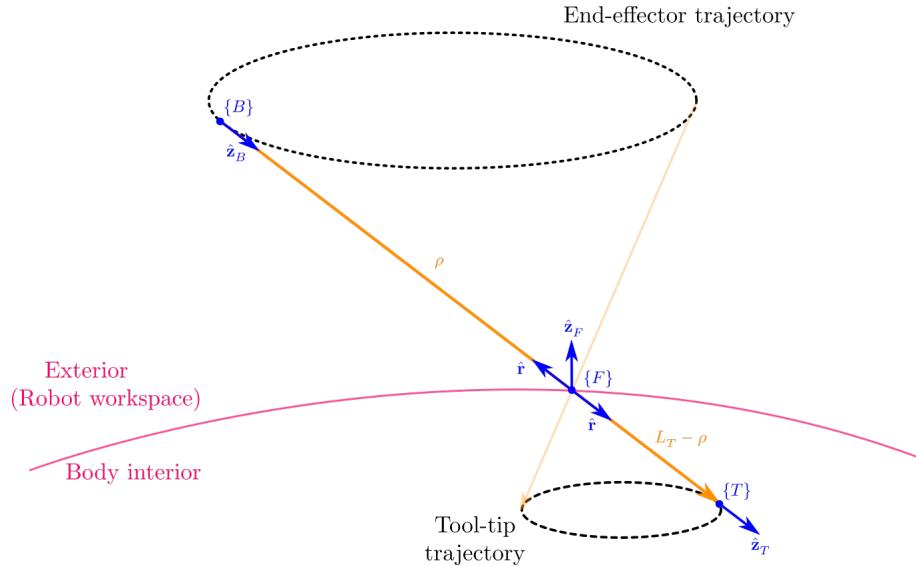


Figure 23: Circular trajectory of tool tip with respect to Fulcrum reference frame

To generate a circular trajectory for the pivot movement we must specify the center of the circle and a vector whose magnitude is the radius of the circle and it's direction gives the orientation of the plane that the circle lies at. The simplest case of a circular trajectory is the one, whose circle lies in a plane parallel to the *xy* plane.

We first consider the motion of the laparoscopic tool tip on a circle parallel to a *z*-plane, with respect to the $\{F\}$ coordinate frame.

$$(x_F - x_{F0})^2 + (y_F - y_{F0})^2 = r_0^2, \quad z_F = z_{F0} \quad (5.2.1)$$

It's often more convenient to express trajectories in a parametric form, which makes it easier to calculate all the waypoints of the trajectory

$$\begin{cases} x_F = r_0 \cos(2\pi s) + x_{F0} \\ y_F = r_0 \sin(2\pi s) + y_{F0} \\ z_F = z_{F0} \end{cases}, \quad s \in [0, 1] \quad (5.2.2)$$

After having calculated the cartesian coordinates we can calculate the spherical coordinates as follows

$$\begin{cases} r = \sqrt{x_F^2 + y_F^2 + z_F^2} \\ \theta = \text{atan2}\left(\sqrt{x_F^2 + y_F^2}, z_F\right) \\ \varphi = \text{atan2}(y_F, x_F) \end{cases} \quad (5.2.3)$$

5.2.2 Circular arc path of tool tip

To generate a circular arc trajectory for a pivot motion we must specify the same parameters as in the circular trajectory as well as the length of the arc or the total angle of the arc section.

5.2.3 Line segment path of tool tip

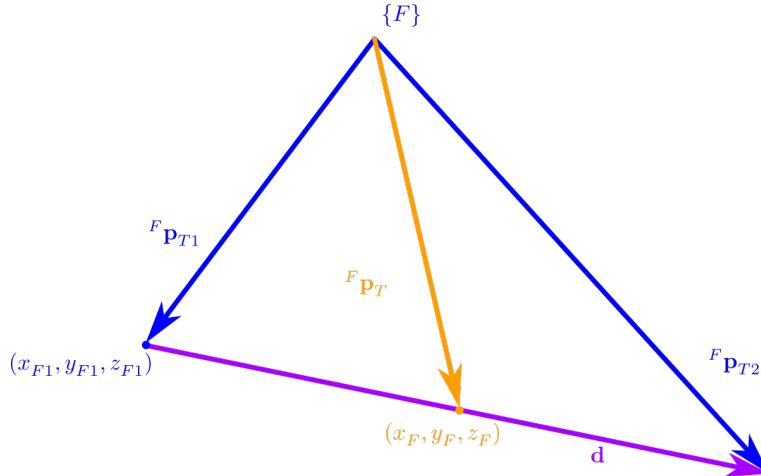


Figure 24: Line segment trajectory of tool tip with respect to Fulcrum reference frame

$$\begin{aligned} \mathbf{d} &= {}^F \mathbf{p}_{T2} - {}^F \mathbf{p}_{T1} = [l, m, n]^\top \\ {}^F \mathbf{p}_T &= [x_F, y_F, z_F]^\top \\ {}^F \mathbf{p}_T &= {}^F \mathbf{p}_{T1} + s \mathbf{d} \\ s &= \frac{x_F - x_{F1}}{l} = \frac{y_F - y_{F1}}{m} = \frac{z_F - z_{F1}}{n} \quad s \in [0, 1] \\ \begin{cases} x_F = sl + x_{F1} = (1-s)x_{F1} + sx_{F2} \\ y_F = sm + y_{F1} = (1-s)y_{F1} + sy_{F2} \\ z_F = sn + z_{F1} = (1-s)z_{F1} + sz_{F2} \end{cases} \end{aligned} \quad (5.2.4)$$

After having calculated the cartesian coordinates we can calculate the spherical coordinates using the 5.2.3 equations.

The line segment trajectory of tool tip, as analysed in this section needs no implementation as it is already implemented in the ROS MoveIt library and can be used by calling the method **computeCartesianPath**.

5.2.4 Cubic Spline path of tool tip

5.2.5 B-Spline path of tool tip

The **B-Splines** are smooth curves which are constructed from **Bézier** curves. A Bézier curve is a parametric smooth curve and is a k -th order interpolation of $k+1$ control points.

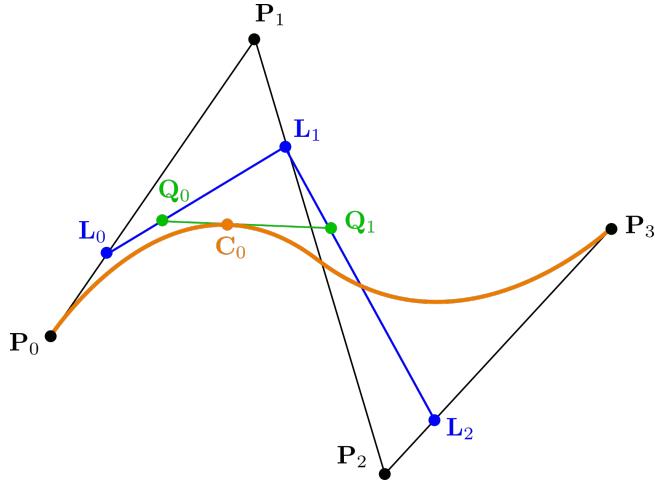


Figure 25: Cubic Bézier curve calculated using cubic interpolation of 4 control points

We first calculate the linear interpolation of the control points

$$\mathbf{L}_0(s) = (1 - s)\mathbf{P}_0 + s\mathbf{P}_1 \quad (5.2.5)$$

$$\mathbf{L}_1(s) = (1 - s)\mathbf{P}_1 + s\mathbf{P}_2$$

$$\mathbf{L}_2(s) = (1 - s)\mathbf{P}_2 + s\mathbf{P}_3$$

The next step is to calculate the quadratic interpolation of the control points or equivalently, the linear interpolation of the previously calculated points $\mathbf{L}_0, \mathbf{L}_1, \mathbf{L}_2$

$$\mathbf{Q}_0(s) = (1 - s)\mathbf{L}_0(s) + s\mathbf{L}_1(s)$$

$$\mathbf{Q}_0(s) = (1 - s)^2\mathbf{P}_0 + 2(1 - s)s\mathbf{P}_1 + s^2\mathbf{P}_2 \quad (5.2.6)$$

$$\mathbf{Q}_1(s) = (1 - s)^2\mathbf{P}_1 + 2(1 - s)s\mathbf{P}_2 + s^2\mathbf{P}_3$$

Similarly for the last step, we calculate the cubic interpolation of the control points or equivalently, the linear interpolation of the previously calculated points $\mathbf{Q}_0, \mathbf{Q}_1$

$$\mathbf{C}_0(s) = (1 - s)\mathbf{Q}_0(s) + s\mathbf{Q}_1(s)$$

$$\mathbf{C}_0(s) = (1 - s)^3\mathbf{P}_0 + 3(1 - s)^2s\mathbf{P}_1 + 3(1 - s)s^2\mathbf{P}_2 + s^3\mathbf{P}_3 \quad (5.2.7)$$

The cubic Bézier curve can also be calculated using the following more compact equation, in matrix form

$$\mathbf{C}_0(t) = [\mathbf{P}_0 \quad \mathbf{P}_1 \quad \mathbf{P}_2 \quad \mathbf{P}_3] \begin{bmatrix} -1 & 3 & -3 & 1 \\ 3 & -6 & 3 & 0 \\ -3 & 3 & 0 & 0 \\ 1 & 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} s^3 \\ s^2 \\ s \\ 1 \end{bmatrix} \quad (5.2.8)$$

A k -degree **B-Spline** curve defined by $n + 1$ control points will consist of $n - k + 1$ Bézier curves. For example if we want to construct a cubic B-Spline using 6 control points, then we will need to construct and connect together 3 Bézier curves.

5.3 Task space analysis

Dexterity analysis for tool's task space

$$\mathcal{D} = \mathcal{L}_q \mathcal{M} \quad (5.3.1)$$

where

$$\mathcal{M} = \sqrt{\det(JJ^\top)} \quad (5.3.2)$$

$$\mathcal{L}_q = 1 - \exp \left\{ -\kappa \prod_{i=1}^{n_k} \frac{(q_i - q_{i,\min})(q_{i,\max} - q_i)}{(q_{i,\max} - q_{i,\min})^2} \right\} \quad (5.3.3)$$

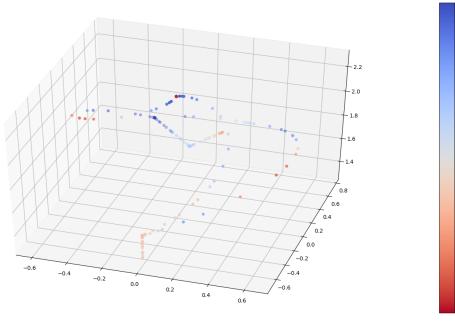


Figure 26: Plot the manipulability of the robot arm at sample points of the executed trajectory

The equation 5.3.3 calculates a joint limit measure which is multiplied with the manipulability measure and gives the dexterity measure. From that equation we can conclude the following:

- If $q_i = q_{\min}$ or $q_i = q_{\max}$ then the exponential is equal to 1 which means that \mathcal{L}_q and \mathcal{D} are both 0, which means that the robot has **no dexterity at the boundary of the task space**.
- If the value of q_i is close to it's boundary value then the dexterity approaches 0. The how much close or far it is from the boundary (or in other words how fast the exponential term converges) depends on the parameter κ
- The q_{\min}, q_{\max} are calculated from the geometry of the task-space

For maximum dexterity at most points of a trajectory in a pivoting motion, the pivot sub- taskspace (i.e. the space of all configurations of feasible pivot motions) must be fully within the robot's whole reachable taskspace, otherwise only a small range of pivot movements will be feasible.

5.4 Sampling methods

The path planning algorithms that were mostly used in this thesis belong to the category of sampling methods. These methods use random functions to choose a sample from the configuration space or the state space. Sampling methods differ from the deterministic grid methods which, which discretize the whole space. Sampling methods are less computationally expensive than the grid methods, but they do not deliver optimal solutions like the latter.

5.4.1 RRT Algorithms

The **Rapidly-exploring Random Trees** algorithm is a sampling planning method that searches for an obstacle-free motion plan from an initial state x_{init} to a set of goal states \mathcal{X}_{goal} . We refer to a set of goal states, because apart from the one desired goal state there can be other neighbor states that are within the allowed position and orientation tolerances.

Algorithm 1: RRT Algorithm

```

foreach replanning attempt do
    initialize vertices  $V \leftarrow \{x_{init}\}$ ;
    initialize edges  $E \leftarrow \emptyset$ ;
    initialize search tree  $T \leftarrow (V, E)$ ;
    while time  $\leq maxPlanningTime$  do
         $x_{rand} \leftarrow \text{getSampleStateFrom}(\mathcal{X})$ ;
         $x_{nearest} \leftarrow \text{getNearestNodeInTreeToState}(T, x_{rand})$ ;
         $x_{new} \leftarrow \text{findLocalPlanFromTo}(x_{nearest}, x_{rand})$ ;
        if  $\text{isPathCollisionFree}(x_{nearest}, x_{rand})$  then
             $V \leftarrow V \cup \{x_{new}\}$ ;
             $E \leftarrow E \cup \{(x_{nearest}, x_{rand})\}$ ;
            if  $x_{new} \in \mathcal{X}_{goal}$  then
                return SUCCESS and path plan  $T = (V, E)$  ;
            end
        end
    end
end
return FAILURE and  $T = (V, E)$  ;

```

Other variations of the RRT Algorithm, which are also available in the OMPL library, included in the MoveIt library of ROS framework are:

- **TRRT** Transition-based RRT
- **BiTRRT** Bidirectional Transition-based RRT
- **RRT***
- **RRTConnect** with is the default OMPL path planner in ROS
- **LBTRRT** Lower Bound Tree RRT

5.4.2 PRM Algorithms

The **Probabilistic Roadmap** (PRM) algorithm is a sampling planning method that constructs a roadmap representation of \mathcal{C}_{free} before searching for a solution. After the roadmap is successfully built, then the algorithm searches for a solution using a traditional graph-based search algorithm. A very important aspect of this algorithm is how the sampling of the free configuration space will be done. The sampling is usually performed using a uniform distribution except from the regions close to

objects where the sampling is more dense.

Algorithm 2: PRM roadmap construction (preprocessing phase)

```

initialize vertices  $V \leftarrow \{x_{init}\}$ ;
initialize edges  $E \leftarrow \emptyset$ ;
initialize roadmap graph  $G \leftarrow (V, E)$ ;
for  $i = 1, \dots, n$  do
     $x_{rand,i} \leftarrow \text{getSampleStateFrom}(\mathcal{X})$ ;
     $\mathcal{N}(x_{rand,i}) \leftarrow \text{getKNearestNeighbors}(G = (V, E), x_{rand,i})$ ;
     $V \leftarrow V \cup \{x_{rand,i}\}$ ;
    foreach  $x \in \mathcal{N}(x_{rand,i})$  do
        if there is no edge between  $x$  and  $x_{rand,i}$  then
            if  $\text{isPathCollisionFree}(x_{nearest}, x_{rand,i})$  then
                 $| E \leftarrow E \cup \{(x_{rand,i}, x), (x, x_{rand,i})\}$ 
            end
        end
    end
end
return  $G = (V, E)$ 

```

Other variations of the PRM Algorithm, which are also available in the OMPL library, included in the MoveIt library of ROS framework are:

- **PRM***
- **LazyPRM**
- **LazyPRM***

5.5 Pick and place algorithm

Algorithm 3: Pick and Place algorithm

```

foreach surgical tool do
    /* Plan the Pick pipeline */  

    set grasp pose;  

    set pre-grasp approach;  

    set post-grasp retreat;  

    set posture of eef before grasp (open gripper);  

    set posture of eef during grasp (closed gripper);  

    /* Plan the Place pipeline */  

    set place location pose;  

    set pre-place approach;  

    set post-grasp retreat;  

    set posture of eef after placing object;  

    Plan pick and place paths;  

end

```

If the pick and place algorithm targets small objects, such as cubes or spheres or other small convex objects then the path planning is straightforward. In the case where, the object to pick and place has at least one dimension that is bigger than the others like a rod or other long objects, such as the surgical tools, used in this thesis, then the path planning becomes more complicated, because of the almost certain collisions of the tool with the links of the rest of the robot (the link of the end-effector will probably not collide with the tool).

6 Trajectory Planning

At this step, given the points of the desired path, a more detailed trajectory is calculated, which will contain all the waypoints that the robot will have to visit. Trajectory planning is executed after a desired path is generated, and consists in mapping the geometric points to specific **time points**, as well as assigning specific **velocities**, **accelerations** and **jerks**, in order to generate the commands needed for the robot controller to execute a smooth motion.

In chapter 5.2, the paths that are calculated are parameterized by the path parameter s . As s increases from 0, the robot moves from the start configuration $q(0)$ to the goal configuration $q(1)$. Path planning outputs geometric information $q(s), s \in [0, 1]$, whereas the **trajectories** that are the subject of this chapter, also include **time information** $q(t), t \in [0, T]$. A path can be converted to a trajectory by defining a function $s(t) : [0, T] \rightarrow [0, 1]$ which maps the time parameter's range to the path parameter's range. This function is also known as **time scaling** or **time parameterization**.

The most common methodology of trajectory planning, which is also used in this thesis, is the one that is studied in the **joint angles space** also known as **configuration space**.

6.1 Trajectory planning in joint angles space

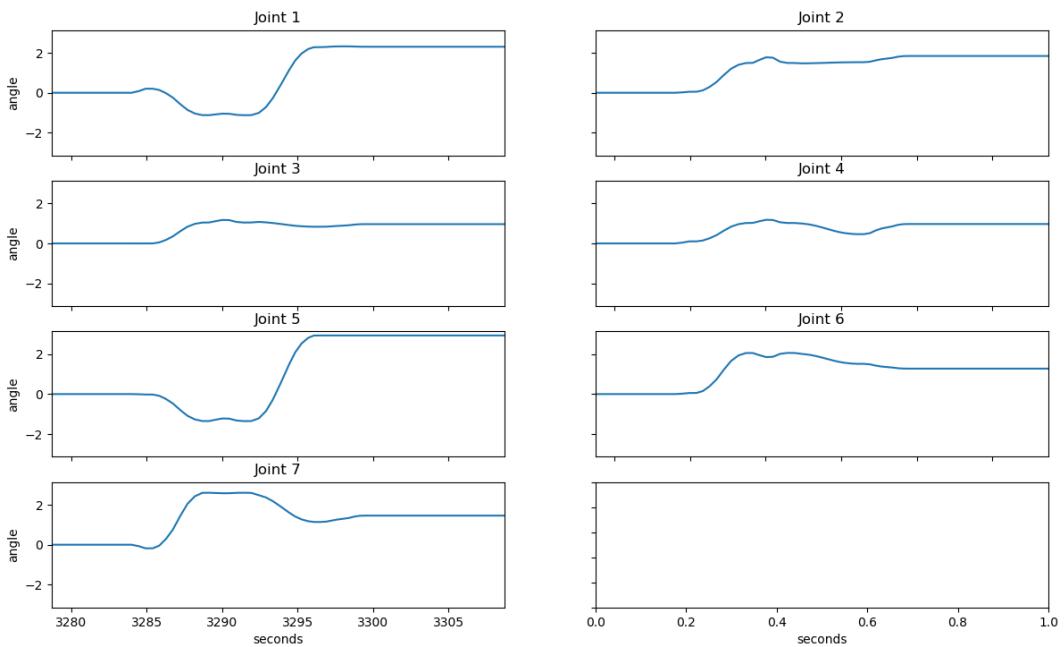


Figure 27: Trajectory diagrams in joints space.

6.1.1 Polynomials of 5th order

6.1.2 Trapezoidal velocity profile

6.1.3 S-Curve velocity profile

6.2 Trajectory planning in cartesian coordinates

Connect the points from path planning with line segments and add more points if needed

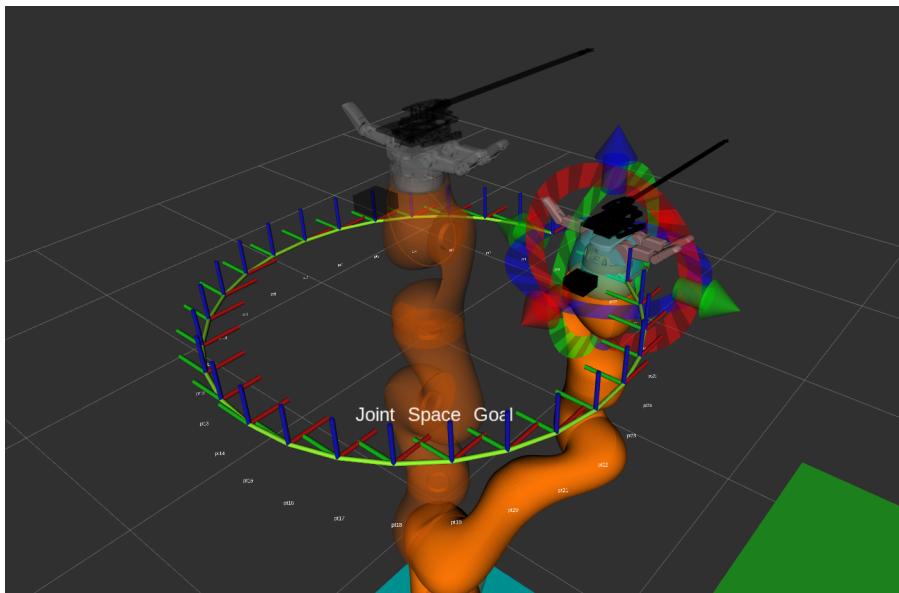


Figure 28: Circular trajectory around the z axis of the home position of the robot

It is very important that the designed trajectory respects the joints angles' range. For example depending on the starting position of the circular trajectory depicted at figure 28, the robot arm may reach it's joint bounds and in order to continue executing the trajectory it will have to make a sudden jump to reset the angles. This could have serious side-effects for both the surgical task and thus the patient, as well as for the operating staff, who control the robot.

7 Implementation with the ROS framework

7.1 Introduction to the ROS framework

ROS is an open-source robotics software framework. It is a meta-operating system, which means that it provides its own abstractions on top of the host's operating system including filesystem, hardware abstractions, low-level device control, package management and networking. It also provides tools and services to develop large, scalable robotics software, it supports a wide variety of libraries and programming languages and it has a huge community, support and documentation resources.

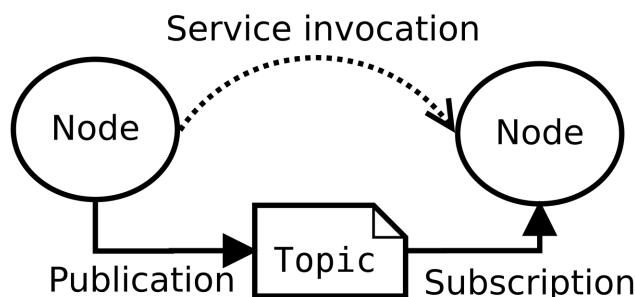


Figure 29: Communication diagram of 2 ROS nodes with a topic and a service

7.2 Gazebo simulation environment

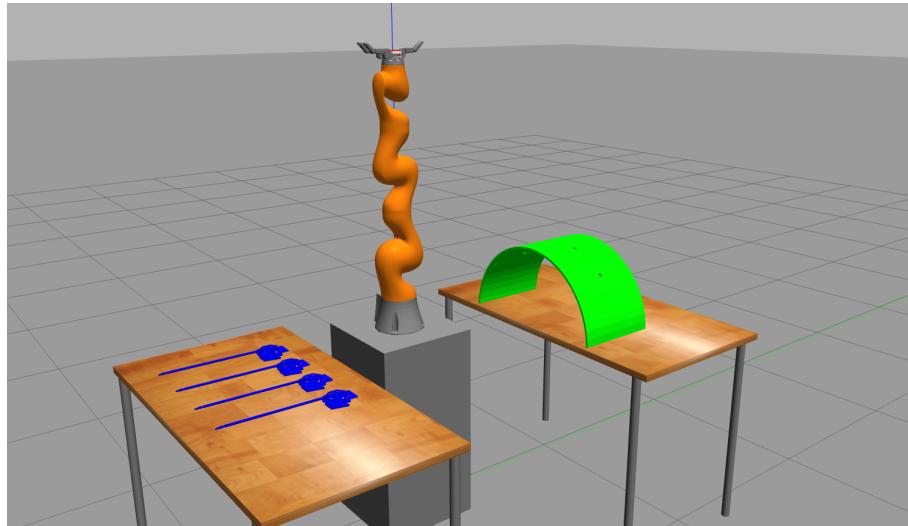


Figure 30: Simulation environment in Gazebo

The main environment setup of this thesis was designed using the Gazebo simulation environment and it consists of the following objects:

- the robot arm, KUKA®iiwa14 lbr, being at the center of the setup
- the robot base, so that the robot arm can better reach the tools and the surgical site and have more flexibility in movement
- 2 tables, one for the tools and one for the surgical site
- 4 surgical tools, using a modified version of the surgical tools used in the Raven II surgical platform
- a mounting dock, which has holes that have the same role as the trocars (small tubes from which the surgical tool is inserted). Initially a mounting dock with 4 same holes of 4mm diameter was used, but it was later replaced with a new one with holes of variable diameters to test feasibility of pivot motions. Larger diameters means more space for motion planner to search for solution and thus more probable to find a solution.

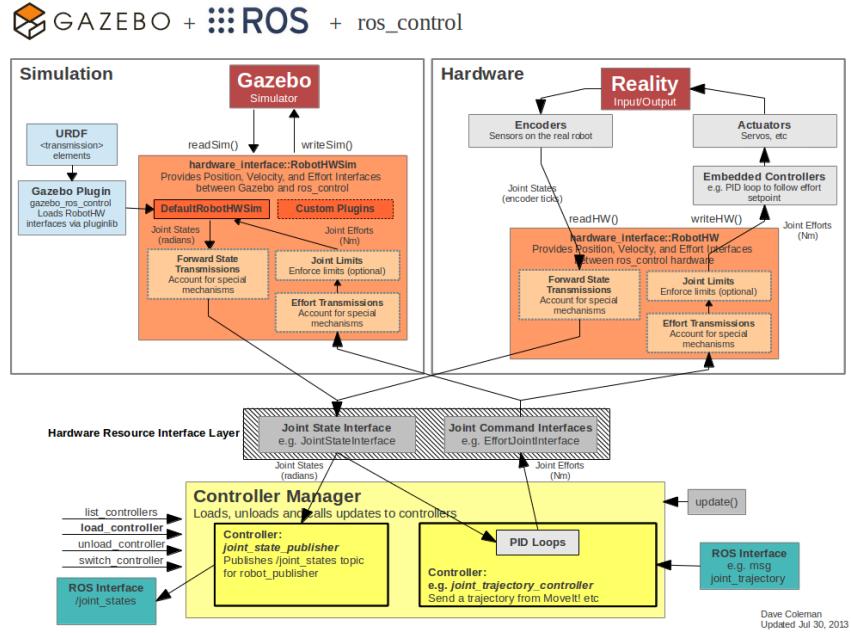


Figure 31: Control & Hardware Interfaces in Gazebo and ROS

7.3 Visualization with RViz

RViz is one of the most important and most used tools in robotic applications development and is a 3D visualizer for the Robot Operating System framework. RViz functionality should not be confused with that of Gazebo, because the first one visualizes the robot state and the **perceived** world (perceived objects or other calculations related to the world) whereas the second one simulates the real world.

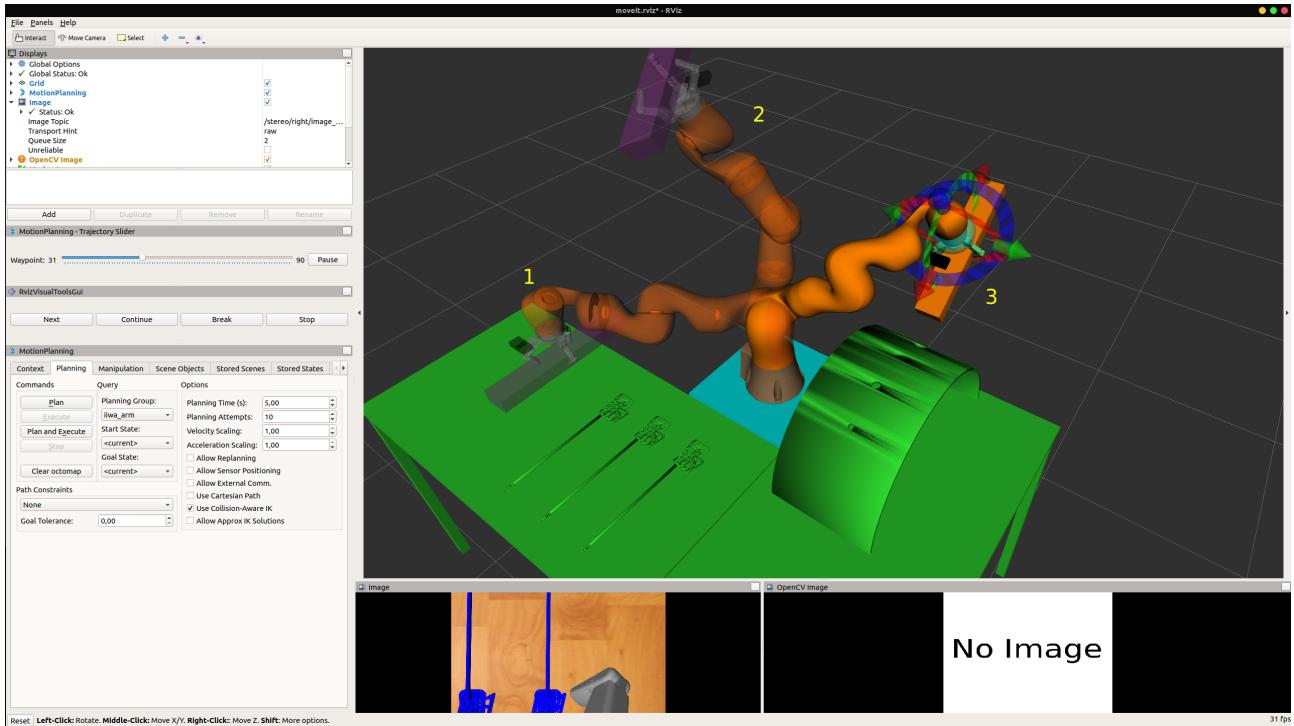


Figure 32: RViz: Visualizing the robot state as well as the state of the perceived world
In this screenshot, various poses of the robot are shown: 1) the current actual real pose of the robot, 2) the planned pose and 3) the goal pose, which can freely be moved within the RViz environment

The objects that appear in RViz can either be visualized from approximations calculated from actual measurements from the robot (for example a point cloud) or can be manually loaded, in which case we make an assumption that the robot already "knows" the exact position, orientation, size and shape of the object, which is rarely the case in real life scenarios. It is important to mention, that every such object is taken into consideration in collision checks and in path planning algorithms.

7.4 Motion Planning with Moveit

When using the Moveit ROS library a set of parameters need to be configured in order to generate the desired commands for the controller:

- **Position tolerance:** The radius of the sphere that the end-effector must reach. This is the maximum allowed error in the target's position. This tolerance is typically much smaller inside the surgical site, to avoid fatalities.
- **Orientation tolerance:** The tolerance or maximum allowed error for roll, pitch and yaw, in radians
- **Maximum planning time:** Maximum amount of time to be used when planning a trajectory
- **Replanning:** Specify whether the robot is allowed to replan if it detects changes in the environment
- **Maximum planning attempts:** Number of times the motion plan is to be computed from scratch before the shortest solution is returned
- **Base frame:** The frame in respect to which the motion plan is calculated.
- **Jump threshold:** This parameter sets an upper bound to the amount of "jump" (change in distance) that can occur between two consecutive trajectory points in joint positions. Disabling

the jump threshold while operating real hardware can cause large unpredictable motions of redundant joints and could be a safety issue

- **Velocity scaling factor:** The approaching motion needs to be slower. We reduce the speed of the robot arm via a scaling factor of the maximum speed of each joint. Note this is not the speed of the end effector point
- **End-effector step:** The resolution at which the Cartesian path is interpolated or the max step in Cartesian translation
- **Planner algorithm:**
- **Fraction:** The fraction of the path achieved as described by the waypoints

Typical motion planning parameter values outside of surgical site:

- Position tolerance: 50 μm
- Orientation tolerance: 0.00005 deg
- Planning time: 10s

Typical motion planning parameter values inside surgical site:

- Position tolerance:
- Orientation tolerance:
- Planning time
- End-effector interpolation step: 1mm
- Maximum velocity scaling factor

Sometimes the motion planner finds a solution but the execution from the controller is aborted. After many iterations of the same experiment this does not happen always, which means that the feasibility of the execution of the movement by the controller depends on the initial state of the robot, i.e. if initially some joints of the robot are at their boundaries, then the next commanded trajectory maybe unfeasible. Another reason that the path planner may fail is the probabilistic nature of the path planning algorithms (see also RRT and PRM algorithms in chapter 6).

At each time step it is important to publish a custom message containing all the information about the kinematic state of the robot. In this thesis a custom **ROS** message was created containing a tf transform with a 3D vector for the position and a quaternion for the rotation and a custom 6-by-7 matrix containing the values of the Jacobian. The MoveIt library, from which the kinematic state of the robot is obtained, returns the orientation of the end effector as a 3-by-3 rotation matrix, but in the ROS tf message it must be expressed as a quaternion. To convert the matrix to a quaternion we first calculate the euler angles and then use these values to construct the quaternion “vector”. The quaternion representation of rotation is often preferred in robotic applications due to its efficiency in calculations and memory. To convert the transformation matrix to euler angles and then to quaternions the following formulas were used:

$$T = \begin{bmatrix} r_{11} & r_{12} & r_{13} & x \\ r_{21} & r_{22} & r_{23} & y \\ r_{31} & r_{32} & r_{33} & z \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$\varphi = \text{atan2}(r_{21}, r_{11})$$

$$\theta = \text{atan2}(-r_{31}, \sqrt{r_{11}^2 + r_{21}^2})$$

$$\psi = \text{atan2}(r_{32}, r_{33})$$

where T is the transformation matrix and φ, θ, ψ are the roll, pitch and yaw (Euler) angles.

7.5 Experiments and Development methodology

7.5.1 Robot Planner 1

In this first experiment we are testing some simple trajectories with the surgical tool already attached to the robot arm's end effector. The path is designed using the appropriate coordinates and orientations so that the robot begins from the home position, then visits the table with the surgical tools and then visits the other table on top of which the mounting dock is placed. Upon arrival at the mounting dock, the robot inserts the tool inside a hole (we consider these holes to be a simplistic alternative to the trocars used in real operations), then executes a simple pivot motion, while the tool is still inserted and then the tool gets ejected from the mounting dock's hole.

The aim of this experiment is to test the overall behaviour of the robot inside the work space, before implementing more complex path planning algorithms.

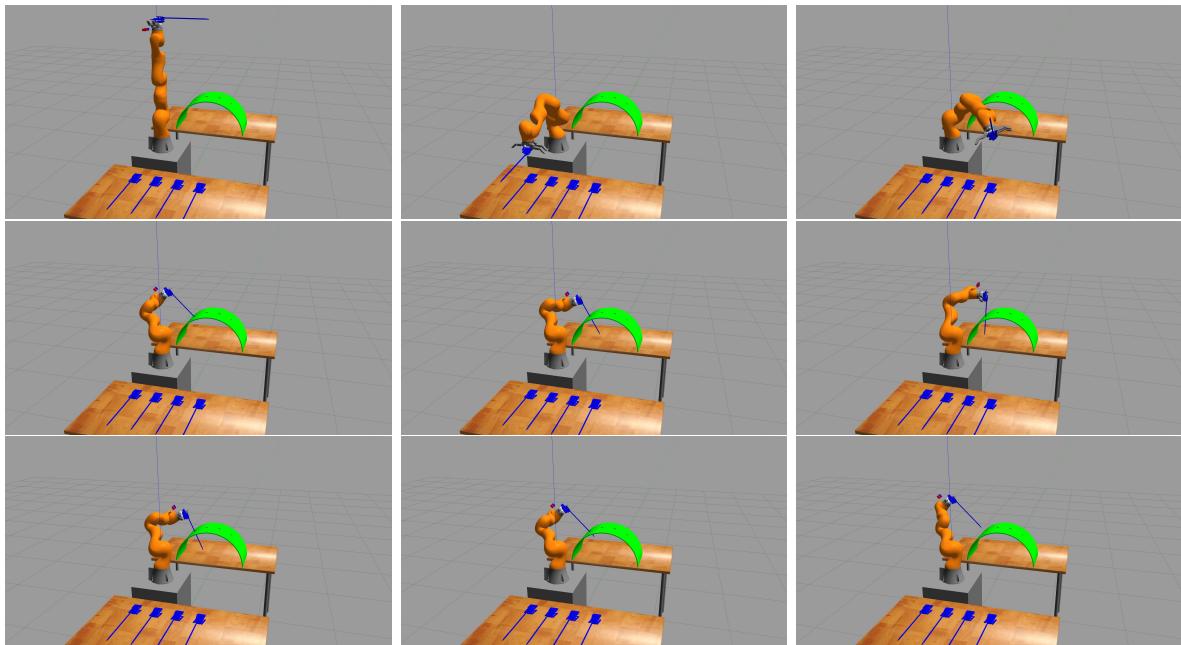


Figure 33: Experiment 1:

7.5.2 Robot Planner 2

In this experiment, we plan a path such that the robot arm will visit all holes of the mounting dock and will try the insertion movement of the surgical tool. This experiment is very useful, because it shows whether all holes of the mounting dock are **reachable** (inside the robot's work space) and if so, how **dexterous** the robot will be in pivoting around each hole, i.e. how free the robot arm is to execute pivot motions.

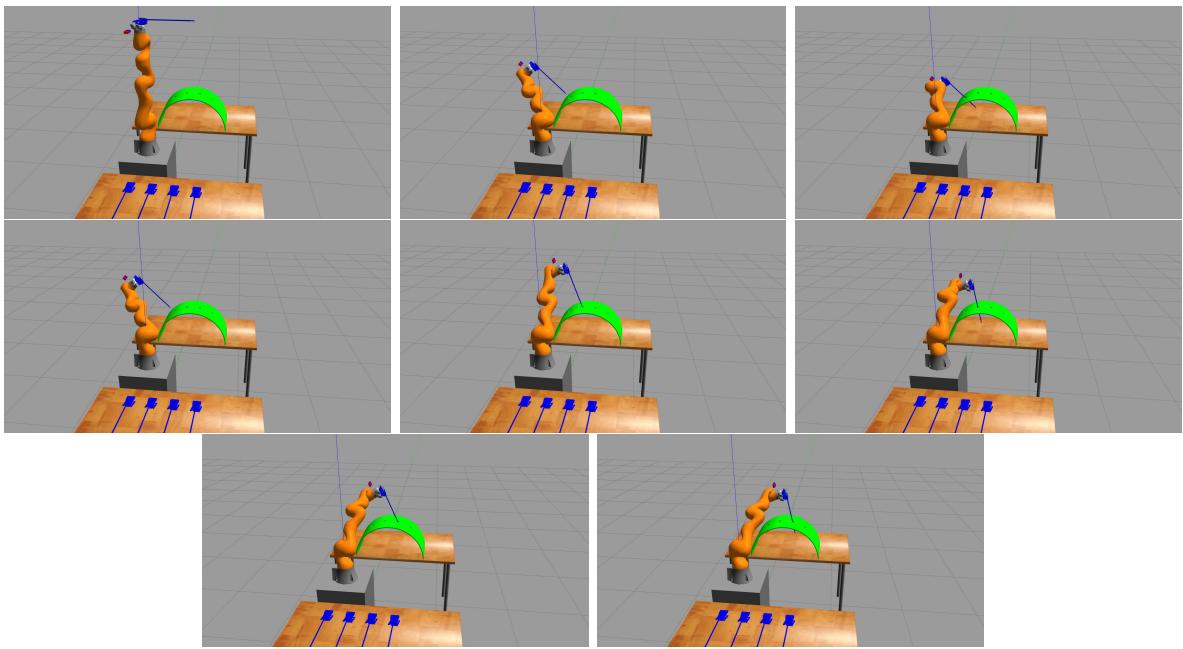


Figure 34: Experiment 2a:

To overcome the reachability issue shown in Figure 34, the algorithm was repeated, but this time using a different simulation layout in Gazebo, in which the mounting dock is closer to the robot and in front of it. This new layout enables the robot to reach all mounting holes with ease and with sufficient dexterity, the robot is free to pivot around.

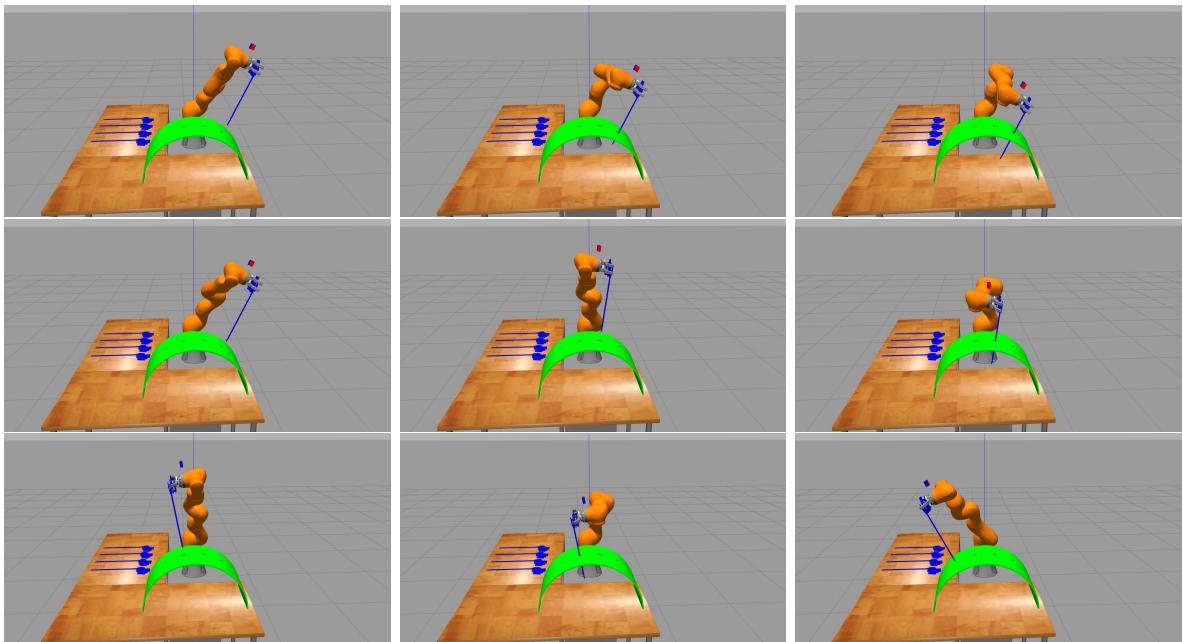


Figure 35: Experiment 2b:

Due to the probabilistic nature of the motion planner (in these experiments the OMPL library is used with the RRTConnect path planning algorithm), the solutions to the path planning problem are not always the same and thus it is possible that the robot arm reaches a pose which is close to a singularity

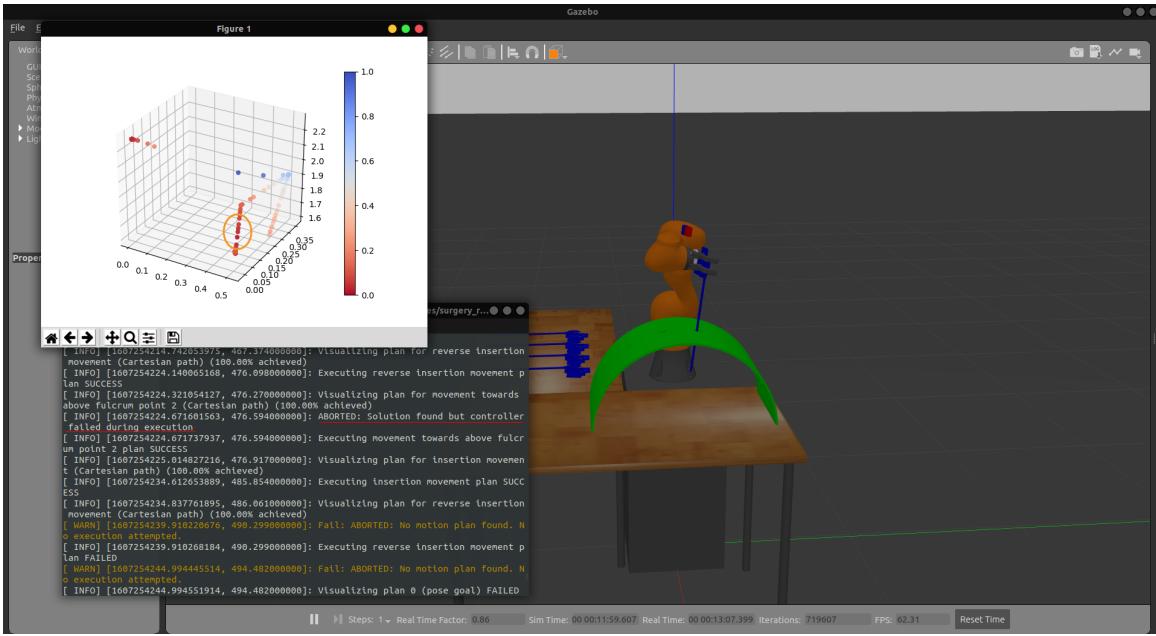


Figure 36: Experiment 2b: Singularity failure

7.5.3 Robot Planner 3

The goal of this third experiment is to design and test only some pivot trajectories. The pivot motions follow the equations described in 5.2. The trajectories that were designed and tested in this experiments are the following:

- Circular
- Arc
- Line segment

7.5.4 Robot Planner 4

In this experiment we plan a simple pick-and-place path for a cube. The robotic arm first visits the left table and starts from the pre-grasp posture and then slowly approaches the cube until the grasp posture. When the gripper has reached the grasp posture, it closes the fingers to grasp the object and then retreats to the post-grasp posture. After that the robotic arm visits the right table to execute the place steps which are similar to the pick steps. The images below show some frames from the experiment with the first three to show the pick steps in the simulation environment and then other three images show the place steps in the visualization program.

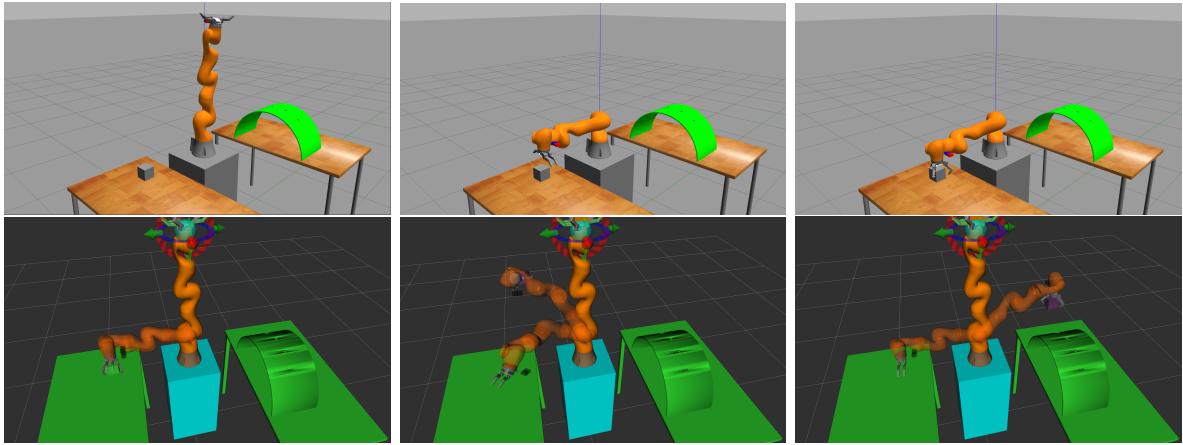


Figure 37: Experiment 4: Simple pick-and-place experiment of a cube

7.5.5 Robot Planner 5

The goal of this fifth experiment is to control the KUKA robot using the camera via the visual servoing technique. In the first part of the experiment the robotic arm goes to an initial known position (e.g. the corner of the table) and then moves around until it detects a surgical tool. When that happens, the image-based visual servoing will send commands to the robot so that the detected tool is at the center of the video frame and with the same orientation as the video frame. At the second part of the experiment, the robot follows a similar algorithm. It starts with a known position, like the corner of the second table, then moves around until the mounting dock starts to appear inside the frame. When that happens, the image-based visual servoing will send commands to the robot so that the center of the trocar or the fulcrum reference frame is at the center and with the same orientation as the video frame. Similar results can be achieved by using position-based visual servoing, but that was not chosen at this implementation for simplicity and less operations. Position-based servoing requires more calculations because it is required to get the camera's transformation, express it with respect to the end-effector and then calculate the end-effector pose which is then used as an input to a Cartesian Controller.

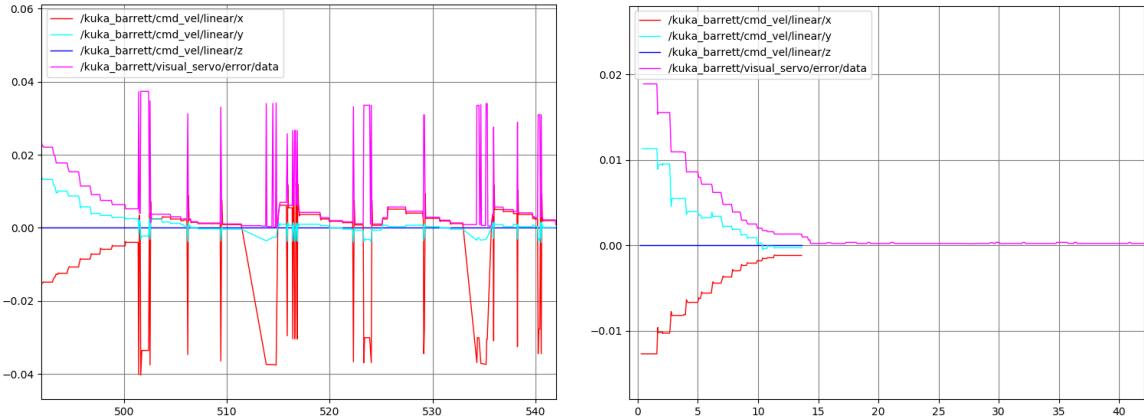


Figure 38: Visual servo controller error diagrams. On the left image in the error graphs appear some spikes. These spikes occur from the sudden temporary detection of a nearby surgical tool. On the right image, these spikes are filtered out, and only the error graphs of the visual servoing of one tool are shown. The controller parameters are $K_p = 0.9$, $K_d = 0.2$

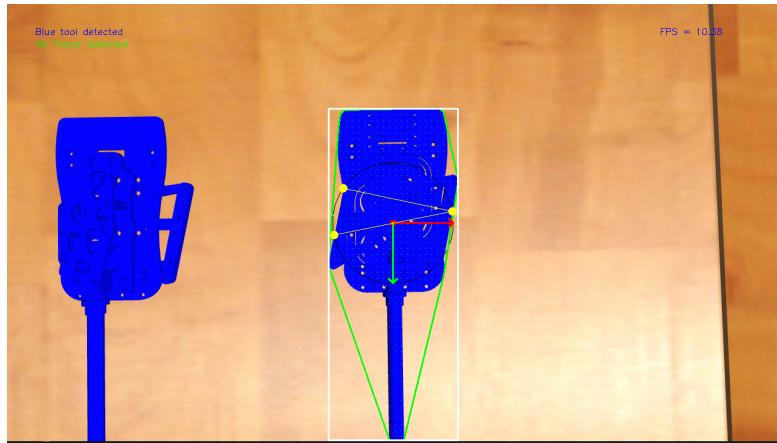


Figure 39: Image based visual servoing and calculation of grasp points. The yellow points are the grasp points and the thin black circumscribed circle is the growing circle that was used to calculate them.

8 Results and Future Work

8.1 Results

Robot Planner 4	PRM*							
	Pick Pipeline				Place Pipeline			
Experiment	Status	Solution Time	Path Simplification Time	Planning Attempts	Status	Solution Time	Path Simplification Time	Planning Attempts
1								
2								
3								
4								
5								
Average								

8.2 Conclusions & Comparison with similar projects

8.3 Future Work

Simulation and interaction with deformable bodies

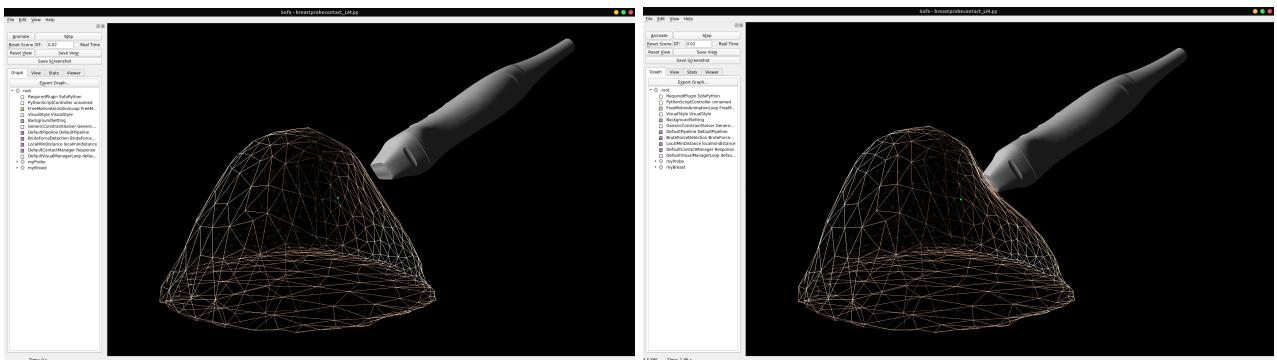


Figure 40: Deformable tissue/organ medical simulation - Simulation of breast probing using the SOFA Framework. Screenshots from running the repository at <https://gitlab.com/altairLab/probe-tissue-simulation>

Advanced visualization and Haptics feedback

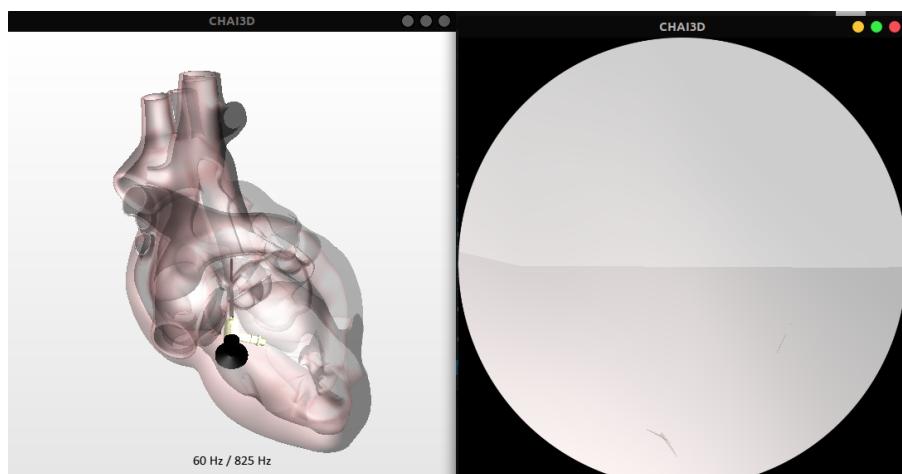


Figure 41: Heart endoscopy medical simulation using the CHAI3D framework. Screenshots from running the repository at <https://github.com/chai3d/chai3d>

Applications of Machine Learning in Computer Vision and Path Planning

Appendices

A Software and Documentation

- All software that developed for this thesis is available and will be maintained at https://github.com/karadalex/surgery_robotics_kuka_barrett
- Instruction on how to run the software of this thesis, as well as documentation of the various software components is available and will be maintained at https://karadalex.github.io/surgery_robotics_kuka_barrett/

B Mathematics

B.1 Euler angles to Quaternions

Let θ, ϕ, ψ be the Euler angles (roll, pitch, yaw) respectively, then using the following equations

$$c\theta = \cos\left(\frac{\theta}{2}\right), s\theta = \sin\left(\frac{\theta}{2}\right)$$

$$c\varphi = \cos\left(\frac{\varphi}{2}\right), s\varphi = \sin\left(\frac{\varphi}{2}\right)$$

$$c\psi = \cos\left(\frac{\psi}{2}\right), s\psi = \sin\left(\frac{\psi}{2}\right)$$

we can calculate the associated quaternion, in vector notation, as follows

$$\mathbf{q} = \begin{bmatrix} q_x \\ q_y \\ q_z \\ q_w \end{bmatrix} = \begin{bmatrix} s\theta c\varphi c\psi - c\theta s\varphi s\psi \\ c\theta s\varphi c\psi + s\theta c\varphi s\psi \\ c\theta c\varphi s\psi - s\theta s\varphi c\psi \\ c\theta c\varphi c\psi + s\theta s\varphi s\psi \end{bmatrix}$$

Nomenclature

$\hat{\mathbf{r}}, \hat{\boldsymbol{\theta}}, \hat{\boldsymbol{\phi}}$ Unit vectors of r, θ, φ axes respectively, in spherical coordinates

$\hat{\mathbf{x}}, \hat{\mathbf{y}}, \hat{\mathbf{z}}$ Unit vectors of x, y, z axes respectively

\mathcal{C} Configuration Space

\mathcal{C}_{free} Free Configuration Space

\mathcal{C}_{obs} Obstacle Space

\mathcal{L}_q Dexterity measure of the robotic arm

\mathcal{M} Manipulability measure of the robotic arm

θ, ϕ, ψ roll, pitch, yaw angles, also known as the Euler angles

${}^{i-1}\mathbf{p}_{iO}$ Position vector from the origin of the coordinate frame $\{i\}$ to the origin of the coordinate frame $\{i - 1\}$

${}^{i-1}R_i$ Rotation matrix from coordinate frame $\{i\}$ to coordinate frame $\{i - 1\}$

${}^{i-1}T_i$ Transformation matrix from coordinate frame $\{i\}$ to coordinate frame $\{i - 1\}$

c_i Shorthand notation for $\cos\theta_i$

J^\dagger Pseudoinverse of the Jacobian

s_i Shorthand notation for $\sin\theta_i$

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