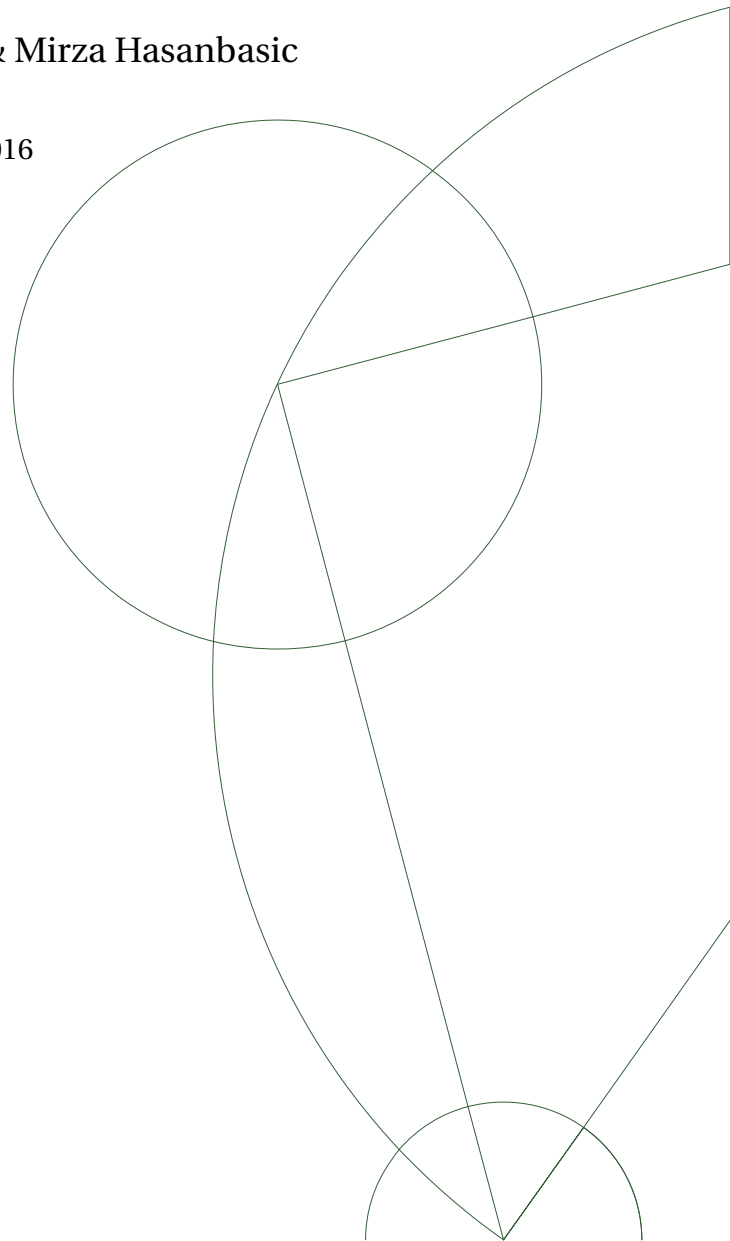




MR Image texture analysis applied to the diagnosis of Alzheimer's Disease

Mathias Bjørn Jørgensen & Mirza Hasanbasic

10th June 2016



Contents

1	Introduction	3
1.1	Problem Definition	3
2	Data	4
2.1	ADNI data	4
2.2	Preprocessing	4
3	Method	6
3.1	Image texture analysis methods	6
3.1.1	Co-occurrence matrix	6
3.1.2	Texture features from co-occurrence matrix	8
3.2	Machine learning	9
3.2.1	10-fold cross-validation	9
3.2.2	Feature selection	9
3.2.2.1	Naive	10
3.2.3	K Nearest Neighbors algorithm	10
3.3	Erode	11
4	Implementation	14
4.1	GLCM Features	14
5	Result	15
6	Discussion	16
7	Conclusion	17
	Appendices	18
A	Co occurrence matrix derivation features	19
	Litteratur	21

List of Figures

3.1	Example of the offsets for the 2D	7
3.2	Image I that is 4-by-4	7
3.3	Four different COM's for a gray-tone image. Shows how the GLCM are calculated of the 4-by-4 image I 3.2.	7
3.4	Example of the offsets for the 3D	8
3.5	The KNN grows a spherical region until it encloses k training samples, and labels the test point by a majority vote of these samples. In this $k = 5$ case, the test point \mathbf{x} would be labelled the category of the black points	11
3.6	Hippocampus at slice 10 on the X-axis as bitwise	12
3.7	Text	12
3.8	Example of a city-block erosion with before and after	12
3.9	2D example of the 3D city-block	13

List of Tables

List of Corrections

Note: find reference	6
Note: level or intensity?	6
Note: rigtigt offset?	6
Note: ændre til $COM_{(0,1)}$... osv	7
Note: Vise for transpose GLCM	7
Note: how does this remove overfitting?	9

Mathias Bjørn Jørgensen & Mirza Hasanbasic

Abstract

This report will examine MRI scans of brains, using image texture analysis and machine learning

Chapter 1

Introduction

Alzheimer's Disease (AD) is the most common cause of dementia among people and is a growing problem in the aging populations. It has a big impact on health services and society as life expectancy increases. In 2010 the total global costs of dementia was estimated to be about 1% of the worldwide gross domestic product¹. AD is the cause in about 60%-70% of all cases of dementia[1] and about 70% of the risk is believed to be genetic [5]. Currently there are no way to cure dementia or to alter the progressive course. But however, much can be done to support and improve the lives if AD is diagnosed in the early stage of progression [1]

In this report we will examine MRI data of the hippocampus using image texture analysis and apply machine learning in order to diagnose AD in patients. Our dataset contain 100 patients 50 control and 50 with AD.

We will be using two different image texture analysis method, one which will me in 2D[7][4] and the other one will be in 3D[9], from which we calculate the data to the gray level co-occurrence matrix (GLCM).

1.1 Problem Definition

Is it possible to classify MRI data of the hippocampus into groups of healthy controls vs Alzheimer's patient, using a predefined set of image texture metrics, with an accuracy greater than 80%?

Is there a difference in diagnosing AD successfully by calculating the co-occurrence matrix in 3D compared to 2D.

¹With the terms as of direct medical costs, direct social costs and costs of informal care

Chapter 2

Data

2.1 ADNI data

The data in this study was provided already downloaded and preprocessed. It had been previously obtained from the ADNI database (adni.loni.usc.edu). The ADNI was launched in 2003 by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, the Food and Drug Administration, private pharmaceutical companies, and nonprofit organizations, as a \$60 million, 5-year, public-private partnership. The primary goal of ADNI has been to test whether serial MRI, positron emission tomography (PET), biological markers, and clinical and neuro-psychological assessments can be combined to measure the progression of MCI and early AD. Determination of sensitive and specific markers of very early AD progression is intended to aid researchers and clinicians to develop new treatments and monitor their effectiveness, as well as to lessen the time and cost of clinical trials. ADNI is the result of efforts of many co-investigators from a broad range of academic institutions and private corporations, and subjects have been recruited from over 50 sites across the U.S. and Canada. For up-to-date information, see <http://www.adni-info.org/> We were provided with a random subset (50 controls, 50 AD) of the “complete annual year 2 visits” 1.5T dataset from the collection of standardized datasets released by ADNI <http://www.adni.loni.usc.edu/methods/mri-analysis/adni-standardized-data/> [11]. The complete dataset (504 subjects) comprised one associated 1.5T T1-weighted MRI image out of the two possible from the back-to-back scanning protocol in ADNI [8] at baseline, 12-month follow-up, and 24-month follow-up.

2.2 Preprocessing

The data were provided for use already preprocessed. This preprocessing, and subsequent hippocampal segmentation was performed with the freely available FreeSurfer software package (version 5.1.0) [6] using the cross-sectional pipeline with default parameters. The original MRI image resolution of $[0.94, 1.35] \times [0.94, 1.35] \times 1.2\text{mm}$ was conformed to a $1.0 \times 1.0 \times 1.0$ mm resolution, and all MRIs were bias field corrected. The bias field correction in FreeSurfer utilizes the nonparametric nonuniform intensity normalization algorithm [10], often

referred to as N3. The input data for this study was therefore the corrected T1-weighted MRI image volume, and corresponding separate binary masks of left and right hippocampi.

Chapter 3

Method

3.1 Image texture analysis methods

Image texture is a feature that can help to segment images into regions of interest and to classify those regions. Textures gives us some information about the arrangement of the intensities in an image. Texture analysis is a technique for evaluating the position and intensity of signal features[4]. Statistical texture analysis methods evaluate the interrelationship of voxels, based on mathematical parameters computed from the distribution and intensities of voxels in the image.

3.1.1 Co-occurrence matrix

The co-occurrence matrix (COM) is second-order statistics methods, which is based on information about colours in pair of pixels. The matrix is defined over the image with distribution values at a given offset. Mathematically we have a COM matrix **C** which is defined over an $n \times m$ image **I**, with $\Delta x, \Delta y$ being the parameterized offset, is calculated by

$$C_{\Delta x, \Delta y}(i, j) = \sum_{p=1}^n \sum_{q=1}^m \begin{cases} 1, & \text{if } I(p, q) = i \text{ and } I(p + \Delta x, q + \Delta y) = j \\ 0, & \text{otherwise} \end{cases}$$

FiXme Note: find reference

The element (5,4) in the COM can be translated to meaning how many times there exist an element in the image with GI **FiXme Note: level or intensity?** 5 and another element offset $\Delta x, \Delta y$ from the original with greyscale intensity¹ (GI) 4, i.e. if the offset is (0,1)**FiXme Note: rigtigt offset?** and the first element is (x,y)(4,3) with GI 5 it would mean that element (x,y)(5,3) would have GI 4. If COM(4,4) is ten, it translates into there being ten instances with element (x,y) = 5 and (x+ Δx ,y+ Δy) = 4. COMs calculated on GIs are often called gray-level co-occurrence matrices (GLCM).

FiXme Note:
find
reference
FiXme Note:
level or
intensity?
FiXme Note:
rigtigt offset?

¹The pixel value is a single number that represents the brightness of the pixel. Typically one is taken to be black and 256 is taken to be white and values in between make up the different shades of grey

A single image have multiple GLCMs as different offsets creates different relations. Consider a 3×3 matrix looking at element (2,2) we can then create eight different offsets, (1,0),(1,1), (0,1)),(-1,1),(-1,0),(-1,-1),(0,-1),(1,-1) **FiXme Note: ændre til $COM_{(0,1)}...$ osv, however they are not unique. FiXme Note: Vise for transpose GLCM**

FiXme Note:
ændre til
 $COM_{(0,1)}...$
osv
FiXme Note:
Vise for
transpose
GLCM

Focusing on the two offsets (0,1), (0,-1) in element (2,2) and (1,2) with GI 1 and 2 respectfully increases the entry $GLCMs_{1,0}(1,2)$ and $GLCMs_{(-1,0)}(1,1)$ with one, showing that $GLCMs_{(0,1)}^T = GLCMs_{(0,-1)}$. There exist the same relation between (1,1)(-1,-1), (0,1)(0,-1), and (-1,1)(1,-1). This leaves four different offsets for analysis (0,1),(-1,1), (-1,0)),(-1,-1) in general (0,d),(-d,d),(-d,0),(-d,-d) where d is the distance which are commonly named angles 0° , 45° , 90° and 135° as seen in figure 3.1.

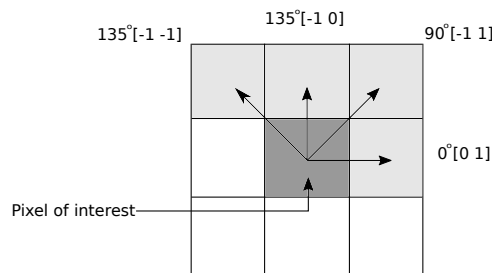


Figure 3.1: Example of the offsets for the 2D

and let figure 3.2 illustrate this concept with a 4×4 image I with four different COM's for $I: C_{(0,1)}, C_{(-1,1)}, C_{(-1,0)}$ and $C_{(-1,-1)}$

I

1	1	4	4
1	1	4	4
3	4	2	2
3	4	2	2

Figure 3.2: Image I that is 4-by-4

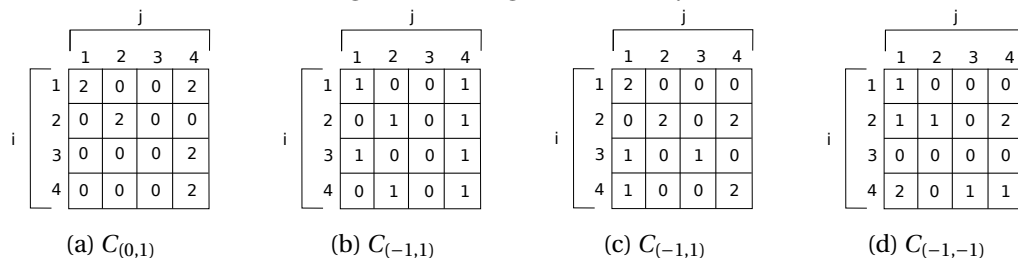


Figure 3.3: Four different COM's for a gray-tone image. Shows how the GLCM are calculated of the 4-by-4 image I 3.2.

The co-occurrence matrix is quadratic with the number of rows and columns equal to the amount of GI, for example if we have 256 GI we get a 256×256 GLCM.

Extending this method to three-dimensions it is necessary to look on how the offsets are defined because the size of the GLCM is defined by the amount of GIs and not by the images it is derived from. Considering a $3 \times 3 \times 3$ matrix we have a possible of 26 offsets. In two-dimensions it is possible to eliminate half of the offsets because of the relation $GLCM_{d,d}^T = GLCM_{-d,-d}$, and it is the same case in three-dimensions with the relation being $GLCM_{d,d,d}^T = GLCM_{-d,-d,-d}$. This leaves 13 offsets which are illustrated below.

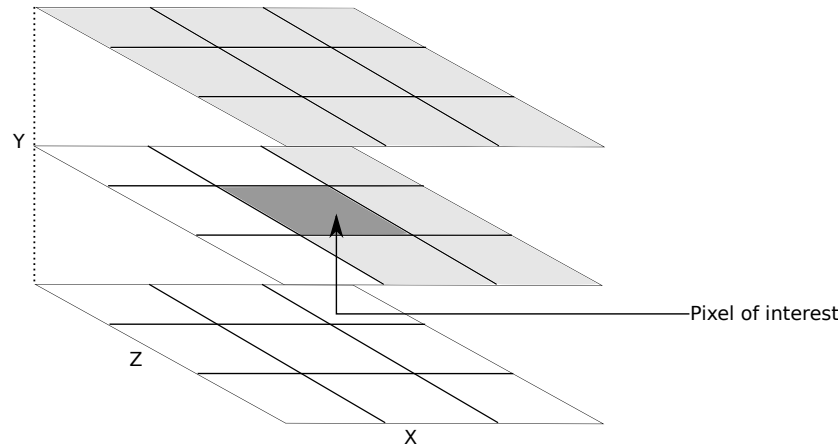


Figure 3.4: Example of the offsets for the 3D

To create a two-dimensional GLCM on three-dimensional image we create slices through the image. Given a $n \times m \times l$, $n = 20$, $m = 20$, $l = 20$, image we can create a slice for each n . $Slice_1$ is equal to the matrix $M(n = 1 \times m \times l)$, $Slice_2 = M(n = 2 \times m \times l)$, and so on, giving a total of 20 $m \times l$ images instead. It is possible for each slice to calculate the $GLCM_{d,d}$ for each slice, and we define $GLCM_{d,d} = \sum_{n=1}^20 GLCM_{d,d}(Slice_n)$

These slices are done in all three directions of the image for the four difference offsets resulting in 12 GLCMs. There is an overlap between six of the GLCMs. Slicing through n axis with offset $(0,d)$ is equal to slicing through the m axis with the same offset. Slicing through the m axis with offset $(-d,d)$ is equal to slicing through the l axis with offset $(-d,0)$. Slicing through the l axis with offset $(-d,d)$ is equal to slicing through the n axis with offset $(d,0)$, which is the transposed offset of $(-d,0)$. Removing the duplicates leaves nine GLCMs which we calculate at distances $d = (1,2,...,10)$, giving a total of 90 GLCMs for each mri scan.

The three-dimensional version is also calculated for distances $d = (1,2,...,10)$ resulting in 130 GLCMs for each mri scan.

3.1.2 Texture features from co-occurrence matrix

To compare the differences between the GLCMs 13 different features are computed. They are the same as used in [7] except for one difference. The difference is how the correlation is calculated as $\sum_{i,j} \frac{(i-\mu_i)(j-\mu_j)glcm(i,j)}{(\sigma_i \cdot \sigma_j)}$, where μ_i , μ_j , σ_i , σ_j are the means and standard deviations of C_i and C_j respectively. This correlation is called the Pearson product moment correlation coefficient and it determines how correlated a pixel is to its neighbour, over the

whole image[2][3]. We calculate two versions of these features, one where we normalized the COMs and one where we do not.

3.2 Machine learning

Short intro to Machine learning

3.2.1 10-fold cross-validation

Given a model with unknown parameters and a training set to which the model can be fit then the fitting process optimizes the model's parameters to fit the training data. Validating this model against independent data (test data) from the same data pool as the training, it will generally turn out that the model does not fit the test data as well as the training data. It is known as overfitting and is a problem when the size of the training data set is small. Cross-validation is used to counteract overfitting.

Dividing the entire data set into 10 groups at random, one subsample is saved for testing and the remaining nine is used to fit the model. The procedure is done so all subsamples get to be used to validate exactly one time and the validation result can then be averaged to produce a single estimation. This solves the problem of overfitting, as the validation data set is never used in to fit the model. **Fixme Note: how does this remove overfitting?**

Fixme Note:
how does
this remove
overfitting?

3.2.2 Feature selection

Feature selection is the process of selection of a subset of relevant features for use in model construction. The main goal of feature selection is to choose a subset of the entire set of input features so the subset can predict the output with an accuracy comparable to using the entire set to predict the output, but with a large reduction in the computational cost. When a dataset contains many features that are either redundant or irrelevant it is possible to remove them without incurring much loss of information. Features may be redundant due to the presence of another feature with which it is strongly correlated, while they may be very informative for the model their information have already been provided by a different feature. Only choosing a subset of the possible features have the added advantage of decreasing the complexity of the model.

Sequential forward feature selection(SFS) is a greedy algorithm to choose features. It starts off with finding the best possible single feature to describe the model. Given the feature set of that single feature, the next step is to find which other feature would improve the predictiveness of the model and then add that to the set of selected features. It continues to grow the set of selected features, until the goal have been reached. The goal can either be a specific amount of features, a specific accuracy for the model or it can stop if all choices of a new feature would decrease the accuracy. A problem with SFS is due to its greedy nature, there is no guarantee that the first feature selected is part of the optimal solution. Given three features X_1 , X_2 and X_3 where X_1 is the best single feature, X_2 is second best and X_3 the worst, it does not necessitate that pairing X_1 , X_2 is better than X_2 , X_3 , nor does it secure any other relation,

meaning that the SFS does not guarantee the optimal solution. Which leads to one of the drawbacks of this feature selection, if a feature is selected it is not possible to exclude it later even if it would increase the evaluation score to do so.

```
1 The algorithm for SFS with 10-fold cross validation
2 Step 1:
3 Set selected features  $Y = \emptyset$ 
4  $X =$  entire featurset
5 Seperate dataset into 10 folds of equal size with 5 of each class,  $\{K_1, K_2, \dots, K_{10}\}$ .
6
7 Step 2:
8 For feature  $i = 1$  to No. of features
9   for fold  $j = 1$  to No. of folds
10     Train a k-nn model on  $\{Y, X_i\}$  using fold  $K_1, \dots, K_{10} \setminus K_j$  as training
11     Calcualte missclassification error of model on  $K_j$ 
12 Average the error for all 10 folds.
13
14 Step 3:
15  $F =$  feature with lowest error
16  $X = X \setminus F$ 
17  $Y = Y \cup F$ 
18
19 Step 4:
20 Continue step 2–3 until the missclassification error worsen or 15 features have been
    → selected.
```

The algorithm is run on 10 different k values for the k -nn model, $k = 1, 2, \dots, 10$.

3.2.2.1 Naive

3.2.3 K Nearest Neighbors algorithm

The K Nearest Neighbor (KNN) is a methoed that is used for classification and regression. It should be noted, that KNN is a non parametric lazy learning algorithm, which means that it does not make any assumptions on the underlying data distribution. In other words, it means that the training phase is fast and KNN keeps all the training data. It should be noted that KNN makes decision based on the entire training data set and in the KNN an object is classified by majority vote of its neighbors, with the object being assigned to the class most common amongst its KNN 's. 3.5

Since the training phase is minimal, then it should be noted that the testing phase is very costly for KNN in both memory and time and often it can be a worst case for time needed, since all points might take point in the decision making.

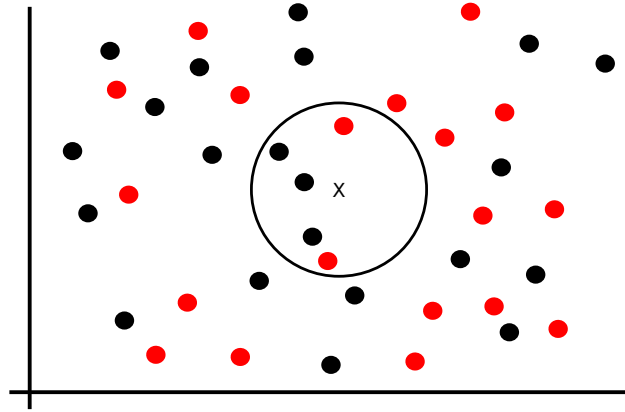


Figure 3.5: The KNN grows a spherical region until it encloses k training samples, and labels the test point by a majority vote of these samples. In this $k = 5$ case, the test point x would be labelled the category of the black points

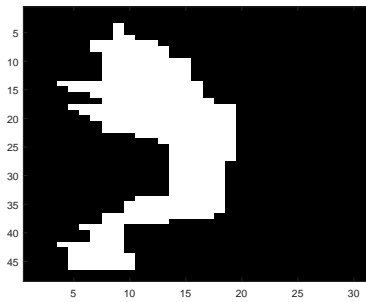
Because the KNN classifier predicts the class of a given test observation by identifying the observations that are nearest to it, the scale of the variables matters. Imagine that we have a large scale variable, they will have a much larger effect on the distance between observations and hence the KNN classifier, than variables on a small scale. Often a good way to handle this problem is to standardize the data.

The disadvantage of KNN is that choosing a k may be tricky, so we are left to test the algorithm on multiple k 's and often it needs a large number of samples for better accuracy.

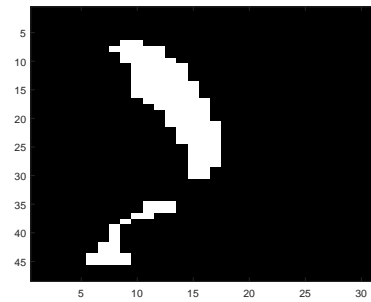
Typically will the KNN classifier be based on a distance, commonly it is based on the Euclidean distance between a test sample and the specified training samples. Let x_i be an input sample with p features $(x_{i1}, x_{i2}, \dots, x_{ip})$, and n be the total number of input samples $i = 1, 2, \dots, n$ and p the total number of features $j = 1, 2, \dots, p$. The Euclidean distance between sample x_i and x_l , $l = 1, 2, \dots, n$ is defined as $d(x_i, x_l) = \sqrt{(x_{i1} - x_{l1})^2 + (x_{i2} - x_{l2})^2 + \dots + (x_{ip} - x_{lp})^2}$

3.3 Erode

Each patient's hippocampus has been segmented in the MRI scan. The problems we can run into are that the background will blur with the segmentation i.e. the hippocampus. Performing an erosion can solve this problem and we can focus on the hippocampus, with the maximum number of details. As seen in figure 3.6a the erosion has not been performed yet, but we might have some problems with data surrounding the hippocampus is blurring out the edges of the hippocampus. To solve this, we create a mask to separate the hippocampus from the background data and end up with what is left in figure 3.6b



(a) Note eroded



(b) After erosion has been performed

Figure 3.6: Hippocampus at slice 10 on the X-axis as bitwise

The erosion we have used is called a city-block metric and can be seen in figure 3.7.

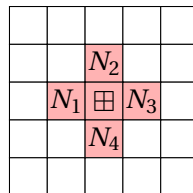
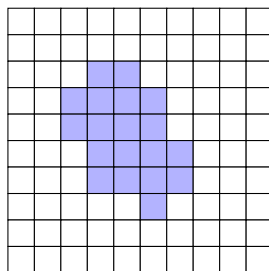
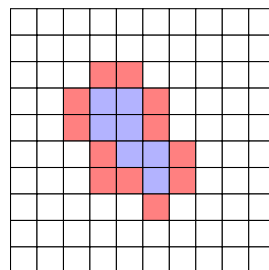


Figure 3.7: Text

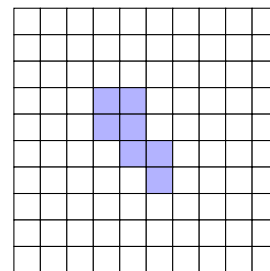
To give an example of how the erosion works, it will be illustrated and we will use the city-block metric for this purpose. So we will use figure 3.7 and erode the image in figure 3.8.



(a) Original image



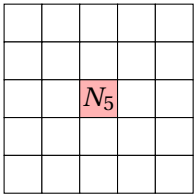
(b) Performing erode on the image



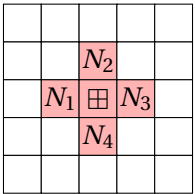
(c) The image after erosion

Figure 3.8: Example of a city-block erosion with before and after

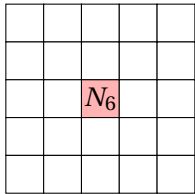
As seen in figure 3.8 the noise (background) have been removed. This is an example in 2D. Now we wish to extend the erosion city-block to 3D. As seen in figure 3.7 it have 4 neighbours and when we extend this to 3D we will end up with 6 neighbours instead as seen in figure 3.9 and the concept is still the same as in 2D



(a) From above



(b) From the front



(c) From below

Figure 3.9: 2D example of the 3D city-block

Chapter 4

Implementation

4.1 GLCM Features

Chapter 5

Result

Chapter 6

Discussion

Chapter 7

Conclusion

Appendices

Appendix A

Co occurrence matrix derivation features

$$C_x(i) = \sum_{j=1}^N C(i, j)$$

$$C_y(i) = \sum_{i=1}^N C(i, j)$$

$$C_{x+y}(k) = \sum_{i=1}^N \sum_{\substack{j=1 \\ i+j=k}}^N, \quad k = 2, 3, \dots, 2N$$

$$C_{x+y}(k) = \sum_{i=1}^N \sum_{\substack{j=1 \\ |i-j|=k}}^N, \quad k=0,1,\dots,N-1$$

$$f_1 = \sum_{i=1}^N \sum_{j=1}^N \{C(i, j)\}^2 \quad (\text{A.1})$$

$$f_2 = \sum_{n=0}^{N-1} n^2 \{C_{x+y}(k)\} \quad (\text{A.2})$$

$$f_3 = \frac{\sum_{i=1}^N \sum_{j=1}^n i j C(i, j) - \mu_x \mu_y}{\sigma_x \sigma_y} \quad (\text{A.3})$$

$$f_4 = \sum_{i=1}^N \sum_{j=1}^N (i - \mu)^2 C(i, j) \quad (\text{A.4})$$

$$f_5 = \sum_{i=1}^N \sum_{j=1}^n \frac{1}{1 + (i - j)^2} C(i, j) \quad (\text{A.5})$$

$$f_6 = \sum_{i=2}^{2N} i C_{x+y}(i) \quad (\text{A.6})$$

$$f_7 = \sum_{i=2}^{2N} (i - f_6)^2 C_{x+y}(i) \quad (\text{A.7})$$

$$f_8 = \sum_{i=2}^{2N} C_{x+y}(i) \log(C_{x+y}(i)) \quad (\text{A.8})$$

$$f_9 = - \sum_{i=1}^N \sum_{j=1}^N C(i, j) \log(C(i, j)) \quad (\text{A.9})$$

$$f_{10} = \text{variance of } C_{x-y} \quad (\text{A.10})$$

$$f_{11} = - \sum_{i=0}^{N-1} C_{x-y}(i) \log(C_{x-y}(i)) \quad (\text{A.11})$$

Bibliography

- [1] Dementia. <http://www.who.int/mediacentre/factsheets/fs362/en/>. Accessed: 2016 April.
- [2] Mathworks graycopros. <http://se.mathworks.com/help/images/ref/graycoprops.html>. Accessed: 2016 May.
- [3] Pearson product. https://en.wikipedia.org/wiki/Pearson_product-moment_correlation_coefficient. Accessed: 2016 May.
- [4] G Castellano, L Bonilha, LM Li, and F Cendes. Texture analysis of medical images. *Clinical radiology*, 59(12):1061–1069, 2004.
- [5] Anne Corbett Carol Brayne Dag Aarsland Emma Jones Clive Ballard, Serge Gauthier. Alzheimer’s disease. *Lancet*, 377:1019–1031, March 2011.
- [6] Bruce Fischl, David H Salat, Evelina Busa, Marilyn Albert, Megan Dieterich, Christian Haselgrove, Andre Van Der Kouwe, Ron Killiany, David Kennedy, Shuna Klaveness, et al. Whole brain segmentation: automated labeling of neuroanatomical structures in the human brain. *Neuron*, 33(3):341–355, 2002.
- [7] Peter A Freeborough and Nick C Fox. Mr image texture analysis applied to the diagnosis and tracking of alzheimer’s disease. *Medical Imaging, IEEE Transactions on*, 17(3):475–478, 1998.
- [8] Clifford R Jack, Matt A Bernstein, Nick C Fox, Paul Thompson, Gene Alexander, Danielle Harvey, Bret Borowski, Paula J Britson, Jennifer L Whitwell, Chadwick Ward, et al. The alzheimer’s disease neuroimaging initiative (adni): Mri methods. *Journal of Magnetic Resonance Imaging*, 27(4):685–691, 2008.
- [9] Rouzbeh Maani, Yee Hong Yang, and Sanjay Kalra. Voxel-based texture analysis of the brain. *PloS one*, 10(3):e0117759, 2015.
- [10] John G Sled, Alex P Zijdenbos, and Alan C Evans. A nonparametric method for automatic correction of intensity nonuniformity in mri data. *Medical Imaging, IEEE Transactions on*, 17(1):87–97, 1998.
- [11] Bradley T Wyman, Danielle J Harvey, Karen Crawford, Matt A Bernstein, Owen Carmichael, Patricia E Cole, Paul K Crane, Charles DeCarli, Nick C Fox, Jeffrey L Gunter, et al. Standardization of analysis sets for reporting results from adni mri data. *Alzheimer’s & Dementia*, 9(3):332–337, 2013.