

Wheeze Detection Using Convolutional Neural Networks

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Abstract. In this paper, we propose to use convolutional neural networks for automatic wheeze detection in lung sounds. We present convolutional neural network based approach that has several advantages compared to the previous approaches described in the literature. Our method surpasses the standard machine learning models on this task. It is robust to lung sound shifting and requires minimal feature preprocessing steps. Our approach achieves 99% accuracy and 0.96 AUC on our datasets.

Keywords: wheeze detection, convolutional neural networks, machine learning, deep learning.

1 Introduction

According to the World Health Organization (WHO), lung diseases are the third most common cause of the death right after the coronary heart disease and stroke. Prevalence statistics of the pulmonary diseases are impressive. For example, in many countries, approximately 5% of the population suffers from asthma, which is appearing as coughing, dyspnea, and the main factor is wheezes.

Wheezes are adventitious sounds present in the lung that is clinically defined as abnormal. Wheezes can be determined as an undesigned and uninterrupted sounds [1]. Lung sound records generated during breathing can be a good source of information for lung treatment. For example, the presence of wheezes in lung sound records of children have been widely used as a parameter to evaluate the inclination to asthma. From an acoustic point of view, wheezes are characterized by periodic waveforms with a dominant frequency usually over 100 Hz [2].

Traditionally, a stethoscope is used to diagnose and monitor wheezes. Stethoscope is a fast, reliable, non-invasive instrument for diagnosing respiration functions of patients. But due to the fact of the increasing number of patients with asthma and other lung diseases, there is a permanent demand for automatic wheeze detection systems. Among other reasons that complicate lung treatment, maybe, the most important one is the late diagnosis. In many countries with low

quality of life, there are simply not enough qualified medical workers to diagnose every patient on time. Thus, for patients with lung diseases uninterrupted and automatic monitoring is very important as the day-to-day state monitoring of lung health can provide key information to the medical diagnosis. The automated wheeze recognition system will also allow any member of medical staff to understand if something is wrong with the respiratory cycle of patient, so it would speed up further treatment. Such systems could help to minimize or eliminate human factor mistakes serving as intellectual decision support systems for medical workers.

The scientific advances in signal processing, speech recognition, time series analysis has been very significant lately, so there are a lot of complex and powerful methods to analyze respiratory cycle sounds nowadays. However, the necessary quality level has not been achieved yet preventing widespread of such systems in real clinics. One of the main problems of most previous studies in wheeze detection is that almost all the methods used there require a lot of complex preprocessing steps of lung sound records to achieve suitable performance. These preprocessing steps are not robust and are sensitive to internal/external noise and quality of records. For example, conventional machine learning (ML) models such as support vector machine (SVM) or k-nearest neighbors (kNN), if being trained on mel-frequency cepstral coefficients (MFCC) features, will work poorly on shifted lung sounds, because MFCC features by nature are not robust to shifting. But in real clinical applications, it is hard to adjust records so they start and end exactly when they are required to. Also, ML models trained on preprocessed data in such ways may not generalize their performance on different versions of stethoscopes.

Deep learning models [3] have recently showed very promising performance on a range of tasks. It has turned out to be a very efficient tool for image recognition [4–6], nature language processing [7–9] and speech recognition [10–13]. In 2012, a convolutional neural network (CNN) was trained to classify 1.3 million high-resolution images into the 1000 different classes [14]. It achieved top-1 and top-5 error rates of 39.7% and 18.9% on the test data. In the area of sound event recognition [15], CNNs beats other feature extraction algorithms and showed great performance in terms of robustness compared with MFCC.

The goal of this study is suggesting an efficient approach for the wheeze detection problem. We propose approach wheeze detection using convolutional neural network (WDCNN) that solves this problem using more flexible architecture. The proposed approach reaches state-of-the-art performance in wheeze detection task and is robust for shifting records and external noise. The contribution of this paper includes:

- To the best of our knowledge, we are the first who presents CNN-based automatic wheeze detection approach.
- Our CNN-based approach on non-processing normalized data like spectrograms are better in terms of evaluation metrics than other approaches that involved a lot of complex preprocessing steps like applying different filters (FIR, Hamming window, etc.), noise reduction techniques, normalization by

frequencies, different feature extraction techniques (MFCC, SBC, Entropy features), etc.

- Our CNN-based solution achieves 99% accuracy and 0.96 AUC measure.

The rest of the paper is organized as follows. In Section 2, the previous studies related to the topic are summarized. We describe our deep learning approach, data that we used and methods for preprocessing in Section 3. Experiments details are presented in Section 4. Results and performance measures are presented in Section 5. Finally, conclusions are made in Section 6.

2 Related Work

In [16], authors proposed an approach to automatic wheeze detection called Entropy-Based Wheeze Detection (EBWD). On the first stage, digital signal was transformed to domain frequency by commonly used STFT (Short Time Fourier Transform) method. STFT procedure produced the Fourier spectrum for each shorter segment of digital signal. On the second stage, peak detection by masking was applied to identify peaks in the signal. After that the authors empirically estimated that vacancy areas beside the peaks for wheezy breath were much larger than for normal breath. They characterized these discrepancies in signals in terms of informational entropy. On the third stage, several features were extracted with respect to entropy. The authors proposed to use features like the difference between maximum and minimum entropy or their ratio and to perform thus wheeze detection using some threshold on this features. As a result, EBWD was able to identify 85% of wheeze samples based on Microphones (Panasonic WM-64 ON) data.

The authors of another paper [17] have demonstrated how Gaussian Mixture Models (GMM) can be applied to classify respiratory diseases. RALE database and 4 classes (normal, wheeze, crackles and asthma) of lung sounds were used in this research. As the preprocessing steps for digital signals from a stethoscope, the authors applied FIR (Finite Impulse Response) filter followed by FFT (Fast Fourier Transform) algorithm. After that, MFCC (Mel-frequency cepstral coefficients) features were extracted from preprocessed signals. The authors conducted several experiments to evaluate the best number of GMMs in the model and also evaluated the accuracy of their models with and without cross-validation. As a result, their approach obtained average (across all classes) 98.7% accuracy without cross-validation and 52.5% accuracy with cross-validation.

In [18], the authors have used a lot of machine learning methods such as feed-forward multilayer neural network (MLP), random forest (RF), logistic regression (LR), naïve Bayes (NB), support vector machine (SVM) and k -nearest neighbors (kNN) for automated wheeze detection using phonopneumograms from the Internet (called INT dataset) and Dubrovnik General Hospital (DGH) datasets. Their preprocessing stages consisted of applying Yule-Walker filter to reduce the influence of cardiovascular and muscular noise followed by STFT procedure. After that, the commonly used MFCC features were extracted from

the preprocessed signals. Also, the authors experimented with some statistical features using FFT (Renyi entropy, Kurtosis, Spectral Flatness (SF), Skewness, etc.) without using MFCC features. As a result, their approach on statistical features achieved 93.62%, 91.77% accuracies for INT and DGH datasets, respectively, by the best model (NN with 2 hidden layers). On MFCC features, their approach with SVM and kNN models obtained 99% on both datasets. The authors claimed that by properly filtering and preprocessing the entry data, and using MFCC features, the signals recorded in suboptimal conditions can be efficiently processed.

Table 1. The Comparison Table

Author	Year	Processing and feature extraction methods	Classifier	Result
Zhang et al.	2009	Entropy, STFT	Entropy-Based Wheeze Detection (EBWD)	Able to identify 85% wheezes samples and systems have been implemented into wearable sound-based respiration monitoring system.
Mayorga et al.	2010	Finite Impulse Response (FIR) filter, Hamming window, Fast Fourier Transform (FFT), Mel Frequency Cepstral Coefficients (MFCC)	Gaussian Mixture Models (GMM)	Accuracy of 98.7% obtained.
Milicevic et al.	2016	Yule-Walker filter, STFT, FFT, MFCC;	MLP, RF, LR, NB, SVM, kNN	93.62%, 91.77% accuracies for INT and DGH datasets, respectively.
Bahoura et al.	2004	MFCC, Subband Based Cepstral (SBC)	Gaussian Mixture Models (GMM), MLP, Vector Quantization (VQ)	GMM on MFCC successfully classify sounds into two category (wheeze and normal sounds).
Palaniappan et al.	2014	MFCC	SVM, kNN	92.19% and 98.26% accuracies obtained for SVM and kNN, respectively.

GMM method was used for binary classification of normal and wheezing respiratory sounds in [19] as well as in [18]. At the preprocessing stage, the sound data were divided into overlapped frames from which a reduced dimension feature vectors were extracted using MFCC procedure and Subband based Cepstral parameters (SBC). The GMM-MFCC combination was compared with Vector Quantization (VQ) and Multi-Layer Perceptron (MLP) neural networks and the best result was obtained by GMM-MFCC. At the postprocessing stage, smoothing of the score function was applied to include the wheezes duration into the model. This led to the significant performance improvement.

In [20], two common classifiers were applied to the data of three categories: normal, airway obstruction pathology, and parenchymal pathology. The MFCC features were extracted from the data and analyzed by one-way ANOVA (analysis of variance). After that, the features were fed separately into the SVM and kNN classifiers. The obtained accuracies of the classification with the SVM and kNN classifiers were found to be 92.19% and 98.26%, respectively.

The most successful recent papers related to wheeze detection are listed in Table 1. These works presented effective techniques that achieved high accuracy values of the exploited classification methods. The Table reflects differences between the techniques, specifically, it shows which processing, feature extraction methods, and classifiers were applied in each work and to what results it has led.

3 Proposed Approach

3.1 Data

Most authors use lung sound data from different internet databases (e.g. [21]) for their research purposes. Such databases were created foremost for educational aims. Each database usually contains a small amount of samples. Unfortunately, most of these databases consist almost only of sick lung sounds.

We collected several datasets from all over the Internet (e.g. soundtracks from YouTube videos and a other sources, e.g. [21]). Some of founded lung sound samples were too long or too short. The number of such samples was 43. These samples were considered as outliers and were dropped. Resulting dataset consisted of 817 samples with 232 healthy and 585 sick lung respiratory cycles. A 2D spectrograms of several samples are shown in Figure 1.

3.2 Methods

There are many preprocessing techniques and feature extraction methods that can be used for lung sound data. Some of these methods were used as a part of the methodology in the previous studies, which were described in Section 2. Most of the observed methodologies included many complex preprocessing steps [22] followed by feature extraction methods like MFCC. There is a good explanation of how MFCC works in [23] A lot of the proposed preprocessing techniques were explained by the fact that there were many data sources with different

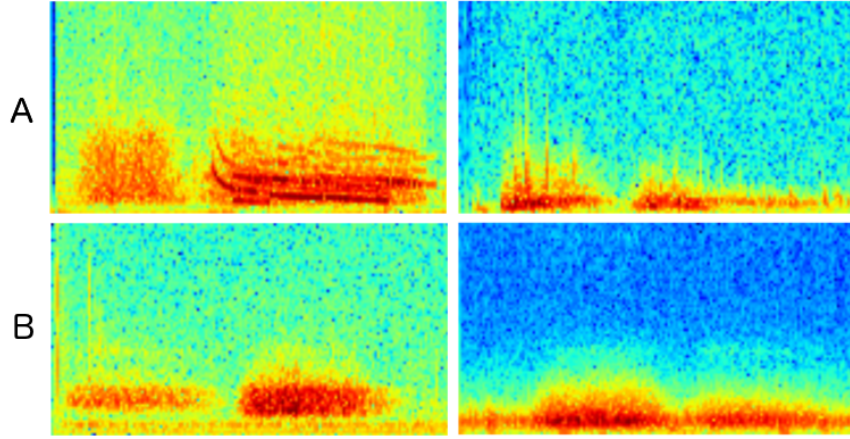


Fig. 1. Examples of respiratory cycle spectrograms. (A) With anomalies. (B) Without anomalies

distributions of frequencies, noises, contents and other characteristics of lung sound data. A methodology has to be insensitive to data changing, data shifting or to some anomalies in the lung sounds. But most of the previously proposed methods were just data cleansing and normalization techniques required to apply machine learning models. For example, finite impulse response (FIR) filter [17] and Yule-Walker filter [18] were used for reducing the impact of noise and for the same frequency range in generated spectrograms by STFT. A classifier required clean normalized data to achieve the better performance score on validation data and to give more stable predictions on the future lung sounds (preprocessed in the same way). In this section, we describe some techniques used in our deep learning approach or used in approaches that we implemented for comparison purposes.

Our deep learning approach for wheeze detection is short and clear. We use a minimum of preprocessing steps and give to CNN almost raw lung sound data. Study design of our approach and CNN scheme is presented in Figure 2.

Data Augmentation is a technique for artificially enlargement of the original data. Deep learning models (such as CNN) require as much data as possible, thus data augmentation is very helpful here to generate new samples and it is also applied to prevent overfitting. Also, due to data augmentation, we can show CNN robustness in terms of respiratory cycle shifting (it is presented in sections 4 and 5 of this paper). Here we consider shifting operation as the biasing of the original lung sound sample by several frames in time.

Data augmentation is the first step of our approach and it is applied to the original data. The soundtracks containing respiratory cycles are shifted several

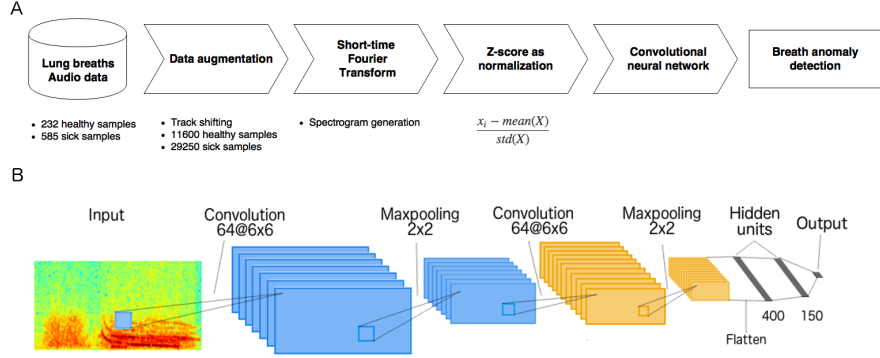


Fig. 2. Deep learning approach. (A) Study design. (B) CNN architecture

times and are marked by id of the original soundtrack. Marking is required to avoid intersection of train and test sets during model training.

The soundtrack shifting technique helps to simulate real-world conditions and to generate many possible variations of specific respiratory cycle. If a classifier can precisely detect anomalies regardless of location of content in the lung sound sample, it is robust enough. For example, a patient can make a mistake and turn on the electronic stethoscope in the middle of the inspiration or turn it off before the end of the cycle.

STFT. Short-time Fourier transform (STFT) is a general-purpose tool for audio signal processing. It is a time-dependent Fourier transform for a sequence, and it is computed using a sliding window. The STFT is a Fourier-related transform that is used to determine the sinusoidal frequency and the phase content of the local sections of a signal as it changes over time.

$$\text{STFT}\{x[n]\}(m, \omega) \equiv X(m, \omega) = \sum_{n=-\infty}^{\infty} x[n] \times w[n - m] \times e^{-j\omega n} \quad (1)$$

where $w[n]$ is the window (frame) and $x[n]$ is the signal to be transformed. The magnitude squared of the STFT yields the spectrogram of the function:

$$\text{spectrogram}(t, \omega) = |\text{STFT}(t, \omega)|^2 \quad (2)$$

which is represented like plots as shown in Figure 1. We use STFT in our approach for obtaining a raw spectrogram of lung sound.

Z-score. It is a normalization technique using formula presented on Fig 3. This type of normalization applies scale on each feature (pixel) of the sample. If we do not scale the input vectors, the ranges of the features (pixels) would likely be different, and this may cause problems related to the specific of gradient based algorithms.

CNN. Convolutional neural network is a type of feed-forward artificial neural network most commonly used for image processing. There is a good explanation of how CNN and its layers work in [24]. Briefly, CNN consists of convolution, pooling and fully connected layers. Convolution layer is a feature extraction part of CNN. It learns filters that are activated when they detect some specific feature (shape) on some position in the input. Max pooling layer is a form of down-sampling. It converts the input image into a set of non-overlapping rectangles and, for each such sub-region, outputs the maximum. Fully connected layers followed by convolutional and pooling layers process high-level abstract features received by learnable convolutions. Also, a fully connected layer is a main building block of regular feed-forward neural network, in which all neurons have full connections to all activations in the previous layer. The output of CNN depends on the task. In our wheeze detection task it is a binary classification problem and there is one neuron in the output of CNN.

4 Experiments

4.1 Experiments design

In this study, we conducted three types of experiments, the only difference in which is the data augmentation application.

- A. A common experiment was conducted on non-augmented data for comparison. Original dataset without data augmentation was used for this experiment. The purpose of this experiment is to compare CNN and other ML models in terms of classification performance.
- B. Each soundtrack was augmented 50 times and then the data were splitted into the train and test sets. There are no augmented copies of any soundtracks from the train set in the test set. The purpose of this experiment is to test CNN and other models for robustness in terms of soundtrack shifting.
- C. This experiment is similar to "B". The only difference is that there are no augmented samples in the train set. The purpose of this experiment is to test whenever or not our CNN-based model holds its generalization ability on shifted samples trained on the original ones.

All experiments were conducted on a computer with Intel Core i7-6900 CPU with 32GB of RAM and NVIDIA 1080 GPU.

4.2 Result evaluation

Due to the unbalanced dataset, we used Area Under Curve (AUC) and Matthews correlation coefficient (MCC) as the performance measures.

AUC score is an area under ROC (receiver operating characteristic) curve. ROC is a graphical plot that illustrates the performance of a binary classifier system as its discrimination threshold is varied. The curve is created by plotting the true positive rate (TPR) against the false positive rate (FPR) at various threshold settings.

MCC is a robust measure for the binary classification task in the case of very different sizes of classes. It returns a value between -1 and +1. A coefficient of +1 represents an ideal prediction, 0 corresponds to no better than a random prediction and -1 indicates the total disagreement between prediction and observation. MCC is calculated using Eq. 3. In this equation, TP is the number of true positives, TN the number of true negatives, FP the number of false positives and FN the number of false negatives.

$$\text{MCC} = \frac{TP \times TN - FP \times FN}{\sqrt{(TP + FP)(TP + FN)(TN + FP)(TN + FN)}} \quad (3)$$

Cross-validation was used to evaluate the results. The idea behind cross-validation is to divide the data set into disjoint training and validation subsets K in different but regular ways, after that a performance measure is evaluated as the mean value on all folds. Thus, results from cross-validation experiments are robust. We used 5-fold cross-validation.

5 Results

5.1 Results of the experiments

The classification performance of different models trained on MFCC features is presented in Table 2. The best result on non-augmented data (MCC 0.88) was achieved by CNN, but MLP, RF and GBM scored just a bit worse (MCC 0.824). In the second (B) and third (C) experiments, CNN completely beat other ML methods in terms of performance and robustness. CNN completely outperformed other models on augmented data, especially when tested on augmented data (0.897 versus 0.32 MCC). CNN robustness in this task is explained by the specificity of model structure. Convolutional layers consist of many learnable filters (feature masks). Filters are independent of content (respiratory cycle) location. Because of this, filters can detect anomalies regardless of soundtrack shifting.

Additionally, Figure 3 shows the performance of classifiers in the form of ROC curves for experiment "B". By analyzing the shown curves, as well as the corresponding AUC score, it can be seen that the best results are achieved by CNN.

Also, we provide results of CNN trained on almost raw features (spectrograms). The results are presented in Table 3. As expected, CNN showed a good feature extraction ability. Our model showed better performance in experiment "B" because of ability of deep learning models to process and memorize big amount of data. Also, we provide loss curve of the best trained CNN for experiment "B". It is shown on Figure 3

Comparison with state-of-the-art models. Almost all the approaches overviewed in Section 2 contained MFCC as the feature extraction step. Performance of our

Table 2. Classification performance received with MFCC features. (A) Original train and test. (B_1) Augmented train and test. (B_2) Augmented train and original test. (C) Original train and augmented test

	A		B₁		B₂		C	
Model	AUC	MCC	AUC	MCC	AUC	MCC	AUC	MCC
SVM	0.787	0.523	0.557	0.095	0.731	0.418	0.5	0
KNN	0.631	0.356	0.531	0.158	0.625	0.331	0.509	0.026
LR	0.79	0.546	0.599	0.134	0.784	0.515	0.505	0.01
GBM	0.874	0.824	0.808	0.279	0.823	0.769	0.507	0.053
RF	0.874	0.824	0.744	0.207	0.77	0.729	0.506	0.091
MLP	0.874	0.824	0.729	0.32	0.866	0.819	0.507	0.061
CNN	0.939	0.88	0.939	0.897	0.931	0.83	0.723	0.519

Table 3. Classification performances of CNN on spectrogram and MFCC features. (MFCC) Augmented train and test. MFCC features were used. (A) Original train and test. Here and below spectrogram features were used. (B_1) Augmented train and test. (B_2) Augmented train and original test. (C) Original train and augmented test

Experiment	Accuracy	F1	AUC	MCC
MFCC	0.961	0.956	0.939	0.897
A	0.989	0.981	0.958	0.916
B₁	0.984	0.977	0.95	0.915
B₂	0.99	0.982	0.96	0.922
C	0.904	0.856	0.772	0.546

approach is 96% of accuracy on MFCC features and 99% on spectrograms. The best accuracy scores were achieved in [17] (98.7%) and in [20] (98.26%). But almost all of the experiments conducted in observed papers used a small data set and were not tested for algorithm robustness.

6 Conclusion

In this paper, we proposed CNN-based approach called WDCNN to detect wheezes in lung sound data. The results showed by the approach on sound signals presented as spectrograms and MFCC features were compared with conventional machine learning models, and WDCNN reaches state-of-the-art performance. Our method outperformed other approaches in the scope in terms of performance measure demonstrating stable 0.96 AUC score on the Internet dataset. Also, several experiments were conducted to prove that WDCNN is the robust method, insensitive to the lung sound shifting and external noise. Our method showed better performance in comparison with the baseline methods.

Our findings showed that the generalization capability and reliability of the proposed CNN-based method is high enough to use it in real-world conditions.

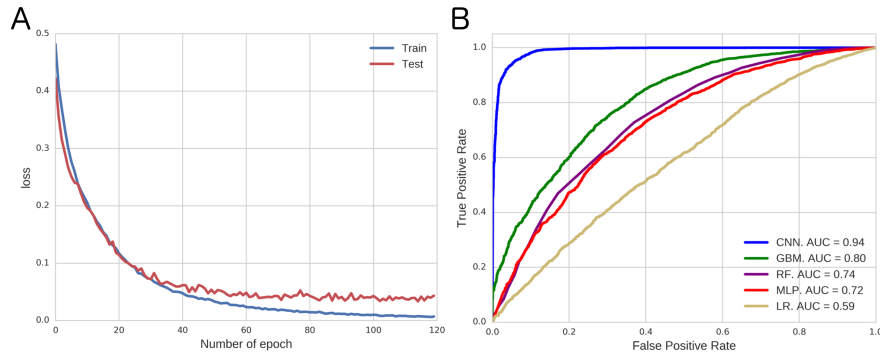


Fig. 3. Performance of best models. (A) Learning curve of the best CNN trained on spectrogram features for "B" experiment. (B) ROC curves for classifiers trained on MFCC features for "B" experiment.

Thus, WDCNN is a well-suited and reliable method to use both in clinics and by any people at home.

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