

Integration of Server- and Embedded System-Based Technology for Dysphagia Data Collection

Nikolay Nechaev, Andrey Somov

I. INTRODUCTION

According to Bloem *et al.* [1], Parkinson's disease is a neurodegenerative disorder with varying symptoms, including bradykinesia, tremor, depression, constipation, disturbed sleep, and cognitive decline. As of 2016, there were 6.1 million people affected by the condition, with that number increasing in the past two decades. One of the Parkinson's disease's symptoms, *dysphagia*, is associated with the death risk of patients experiencing it.

Dysphagia, or swallowing dysfunction, refers to the difficulty or discomfort experienced while swallowing¹. It can affect people of all ages and may be caused by various factors. The severity of dysphagia may vary, ranging from mild discomfort or difficulty to a complete inability to swallow². Dysphagia can lead to reduced food and fluid intake, longer meal times, and less enjoyment of eating and drinking. It may also cause people to avoid social activities such as dining out. Additionally, dysphagia can lead to food or drink entering the airway instead of the esophagus, passing the vocal cords, and entering the lungs, which can be potentially life-threatening. Other consequences include malnutrition, aspiration pneumonia, and even death.

There are several methods to detect Dysphagia. The gold standards are **Video Fluoroscopic Swallow Study (VFSS)** and **fibreoptic endoscopic evaluation of swallowing (FEES)**³. **VFSS** is an evaluation of swallowing function performed using a video x-ray. During this assessment, a Speech and Language Therapist will provide a patient with food and drinks of varying consistency and observe as they swallow it. This enables a therapist to identify and analyze issues with the patient's swallowing, including food going in the wrong direction. **FEES**⁴ is another type of swallow assessment that involves inserting a camera through one's nose to view their throat. A therapist will offer food and drinks, and observe the swallowing process. Similar to **VFSS**, the therapist can detect problems and see if anything is going towards the lungs.

VFSS is an invasive procedure that involves radiation exposure [2] and carries the risk of aspiration of barium bolus [3]. On the other hand, **FEES** is also an invasive procedure that can

impact normal swallowing behavior [4]. It's important to note that VFSS may not always identify neuromuscular abnormalities in pharyngeal or laryngeal physiology [5]. For example, patients with muscle tension dysphagia may exhibit normal oropharyngeal and esophageal swallowing function despite presenting functional dysphagia during a videofluoroscopic swallow study [6], [7].

Researchers apply different combinations of sensors to study swallowing function and dysphagia, such as: an accelerometer with a microphone [8], High-resolution cervical auscultation sensors [9], Surface Electromyography sensors [10], etc. In a previous project⁵ that I worked on we used an MPU6050 accelerometer and a piezoelectric sensor to collect data from a patient during their swallowing. Unlike the previous work, here I focus on the transfer of data between devices involved in the process of measurements collection.

The aim of this project is to design a hardware-software solution to collect data from a patient and store it for later processing. The solution may comprise several parts to reduce the cost of the embedded wearable device and make it more convenient for the patient (e.g., by reducing its weight).

II. RESULTS

The system contains three devices:

- **Wearable device**, comprising an ESP32 microcontroller and sensors, is a lightweight low-performance device that makes measurements and sends them to the Intermediate device via TCP.
- **Intermediate device** is a Raspberry Pi board located on the local network with the Wearable device. It is intended to orchestrate the measurement process: it exposes a user interface to perform measurements, accumulates data sent by the Wearable device, and forwards it to the Server via HTTP.
- **Server** is a remote high-performance device that receives and decodes measurements and stores them for further analysis.

The prototype of the Wearable device comprises an ESP32 microcontroller, an MPU6050 accelerometer, and an AD8232 ECG sensor. For the Intermediate device, I first attempted to

¹<https://www.hopkinsmedicine.org/health/conditions-and-diseases/swallowing-disorders>

²<https://www.nnuh.nhs.uk/departments/speech-and-language-therapy/swallowing/instrumental-swallow-assessment/>

³<https://www.hopkinsmedicine.org/health/treatment-tests-and-therapies/fibreoptic-evaluation-of-fees>

⁴<https://swallowingdisorderfoundation.com/patient-videos/>

⁵<https://github.com/kolayne/dysphagia-project/tree/iot-sem>

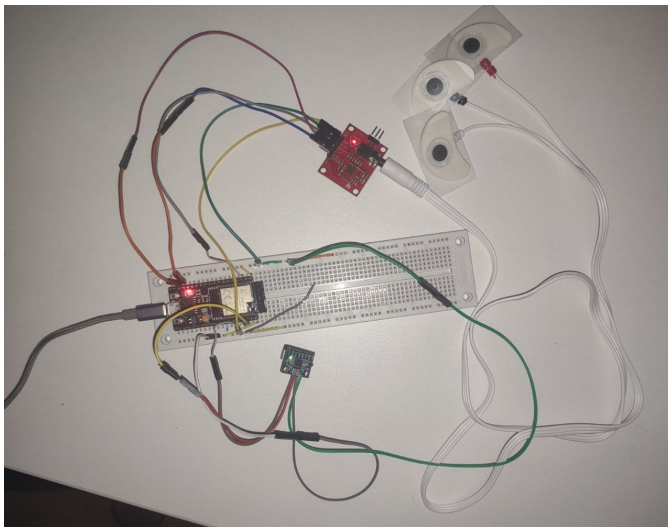


Fig. 1: Wearable device hardware: an ESP32 microcontroller (left), an AD8232 ECG sensor (top), and an MPU6050 accelerometer (bottom)

use an NVidia® Jetson Nano™⁶ board, which, due to its high performance, would be able to collect high-FPS⁷ video feed when connected to a video camera. However, because Jetson Nano lacked built-in wireless capabilities, I selected Raspberry Pi as the Intermediate device board instead.

I implemented the Wearable device firmware in the Arduino programming language⁸ and the Server software in the Python programming language⁹ based on the Flask framework¹⁰. The software solution for the Intermediate device is based on the *ncat*¹¹ and *curl*¹² open-source utilities.

The source code for the Wearable device, the Intermediate device, and the Server is available at <https://github.com/kolayne/dysphagia-project/tree/ERP>.

The implemented system has a high level of reliability: because the Wearable device communicates to the Intermediate device via the TCP protocol, it ensures that measurements are delivered in order and without corruption; in case of connection failure the Wearable device will retry sending data until the Intermediate device is up, so no data is lost.

The Intermediate device, when sending data to the Server, can also detect successful and failed submissions, as well as produce informative logs, which can be made visible in the user interface to make the system more transparent for its users.

```
Could not connect to server, retrying in 100ms
Could not connect to server, retrying in 100ms
Could not connect to server, retrying in 100ms
Could not connect to server, retrying in 100ms
Could not connect to server, retrying in 100ms
Could not connect to server, retrying in 100ms
Connection to server established after 146 attempts
Connection to server established after 0 attempts
Connection to server established after 0 attempts
Connection to server established after 0 attempts
Connection to server established after 0 attempts
```

Fig. 2: Wearable device serial port log: the wearable device started before the Intermediate device was ready, so it keeps sending data until the endpoint is up, then continues normally

```
RPI@RPI3:~$ ADDR=192.168.208.63:5000/measurements ./run.sh
curl: (7) Failed to connect to 192.168.208.63 port 5000: Connection refused
Sent. Response status: 000
curl: (7) Failed to connect to 192.168.208.63 port 5000: Connection refused
Sent. Response status: 000
Sent. Response status: 200
Sent. Response status: 200
Sent. Response status: 200
```

Fig. 3: Intermediate device command-line interface: the Intermediate device started before the Server was ready, so the first two requests failed with the error indicated; further requests succeeded

III. CONCLUSION AND FUTURE WORK

In this project I implemented a prototype of the Wearable device based on the ESP32 controller and developed three software components that chain up devices of the system: the Wearable device firmware that makes measurements and sends them via TCP, the Intermediate device web server that accumulates data sent via TCP and forwards it via HTTP, and the Server-side web server that accepts and decodes measurements sent via HTTP.

Future work on the measurement collection system may continue in the following directions:

- Adding more sensors to the Wearable device to collect more data relevant for analysis;
- Adding more data sources (e.g., connecting a video camera recording the patient);
- Improving security: adding authentication mechanisms to the Intermediate device and the Server, so that only data from the real device is collected and processed.

The results of this project can be used for collection of data from dysphagic patients in further research of dysphagia in neurodegenerative diseases.

REFERENCES

⁶<https://www.nvidia.com/en-us/autonomous-machines/embedded-systems/jetson-nano/product-development/>
⁷https://www.ximea.com/support/wiki/apis/Jetson_Nano_Benchmarks
⁸<https://www.arduino.cc/reference/en/>
⁹<https://python.org/>
¹⁰<https://flask.palletsprojects.com/>
¹¹<https://nmap.org/ncat/>
¹²<https://curl.se/>

[1] B. R. Bloem, M. S. Okun, and C. Klein, "Parkinson's disease," *Lancet*, vol. 397, no. 10291, pp. 2284–2303, Jun. 2021, doi: [10.1016/S0140-6736\(21\)00218-X](https://doi.org/10.1016/S0140-6736(21)00218-X).
[2] Y. Morishima, K. Chida, and H. Watanabe, "Estimation of the dose of radiation received by patient and physician during a videofluoroscopic swallowing study," *Dysphagia*, vol. 31, pp. 574–578, June 2016, doi: [10.1007/s00455-016-9718-6](https://doi.org/10.1007/s00455-016-9718-6).

- [3] M. Iizuka, M. Kobayashi, Y. Hasegawa, K. Tomita, R. Takeshima, and M. Izumizaki, "A new flexible piezoelectric pressure sensor array for the noninvasive detection of laryngeal movement during swallowing," *The journal of physiological sciences*, vol. 68, pp. 837–846, May 2018, doi: [10.1021/acssensors.0c02339](https://doi.org/10.1021/acssensors.0c02339).
- [4] S. G. Hiss and G. N. Postma, "Fiberoptic endoscopic evaluation of swallowing," *The Laryngoscope*, vol. 113, no. 8, pp. 1386–1393, August 2003, doi: [10.1097/00005537-200308000-00023](https://doi.org/10.1097/00005537-200308000-00023).
- [5] M. Vaiman, "Standardization of surface electromyography utilized to evaluate patients with dysphagia," *Head & face medicine*, vol. 3, pp. 1–7, June 2007, doi: [10.1186/1746-160X-3-26](https://doi.org/10.1186/1746-160X-3-26).
- [6] C. H. Kang, J. G. Hentz, and D. G. Lott, "Muscle tension dysphagia: symptomology and theoretical framework," *Otolaryngology–Head and Neck Surgery*, vol. 155, no. 5, pp. 837–842, 2016.
- [7] P. Krasnodebska, A. Jarzyńska-Bučko, A. Szkielkowska, B. Miałkiewicz, and H. Skarżyński, "Diagnosis in muscle tension dysphagia," *Polish Journal of Otolaryngology*, vol. 75, no. 1, pp. 16–22, 2021.
- [8] J. M. Dudik, I. Jestrović, B. Luan, J. L. Coyle, and E. Sejdić, "A comparative analysis of swallowing accelerometry and sounds during saliva swallows," *Biomed. Eng. Online*, vol. 14, no. 1, p. 3, Jan. 2015, doi: [10.1186/1475-925X-14-3](https://doi.org/10.1186/1475-925X-14-3).
- [9] C. Donohue, Y. Khalifa, S. Mao, S. Perera, E. Sejdić, and J. L. Coyle, "Establishing reference values for temporal kinematic swallow events across the lifespan in healthy community dwelling adults using high-resolution cervical auscultation," *Dysphagia*, vol. 37, no. 3, pp. 664–675, Jun. 2022, doi: [10.1007/s00455-021-10317-0](https://doi.org/10.1007/s00455-021-10317-0).
- [10] Y. Ye-Lin, G. Prats-Boluda, M. Galiano-Botella, S. Roldan-Vasco, A. Orozco-Duque, and J. Garcia-Casado, "Directed functional coordination analysis of swallowing muscles in healthy and dysphagic subjects by surface electromyography," *Sensors (Basel)*, vol. 22, no. 12, Jun. 2022.