

FYS3710

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December 17, 2017

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1 The action potential

Characterised by a sharp increase in the membrane potential (depolarisation of the membrane) followed by a less sharp decrease towards the resting potential (repolarisation). This may be followed by an afterhyperpolarisation phase in which the membrane falls below the resting potential before recovering gradually to the resting potential.

The main difference between the propagation of action potentials and passive propagation of signals is that action potentials are regenerative, so their magnitude does not decay during propagation

- 1) experiments are carried out to determine the kinetics of a particular ion-channel
- 2) Create model by fitting equations to results
- 3) Solving the equations and simulate action potentials and other behaviors.

Capacitive current

$$I_c = C_m \frac{dV}{dt}$$

I_{Na} is sodium current, I_K is potassium current, I_L is the leak current.

$$I = I_c + I_i$$

The magnitude of each type of ionic current is calculated by $I_x = g_x(V - E_x)$, $(V - E_x)$ is called the driving force g_x is the conductance for ion x.

2 Models of active ion channels

In chapter 3 we looked at the sodium and potassium voltage-gated ion channels in the squid giant axon. There are many other types of active channels and in this chapter we will look at some methods for modelling the kinetics of voltage-gated and ligand-gated ion channels.

2.1 Ion channel structure and function

Each ion channel is constructed from one or more protein subunits. Those that form the pore within the membrane are called principal sub units.

Picture: Secondary structure of one subunit of a voltage-gated potassium channel. S1 - S6 is polypeptide chains arranged in α - helices (peptides are amino acid monomers linked by peptide bonds). S1 - S4 is voltage-sensitive domain, S5-S6 is the lining of the pore. Hodgkin and Huxley proposed a voltage-sensing mechanism consisting of movement of charged particles within the membrane. This has been confirmed in the S4 segment of the voltage-gated potassium channel VSD. Positive charges(gating charges) in the S4 segment experience an electric force due to the membrane potential. The movement of these gating charges lead to other segments in the channel moving.

There may be one principal subunit (e.g Na^+ and Ca^{2+} channels), or more than one (e.g. in voltage-gated K^+ channels).

More than one principal subunit: Multimers

- Identical: Homomers
- Not identical: Heteromers

Ion channels may also have auxiliary subunits attached to the principal subunits. These subunits may be in the membrane or in the cytoplasm and can change the function of the primary subunits. e.g from inactivating to non inactivating.

Q: How is the structure of one protein subunit-channel?

Q: How is the auxiliary subunit attached? And what is the point of it?

2.2 Ion channel nomenclature

The genes of several channels have been sequenced and each channel is named according to the scheme used for the organism in which it occurs. The prefix of the gene gives some information about the type of channel to which it refers; eg. genes beginning with KCN are for potassium channels.

The IUPHAR naming scheme is commonly used by biophysicists, where the name of the channel begins with the chemical symbol of the principal permeating ion and is followed by a subscript describing the principal regulator or classifier of the channel. E.g Ca_v . We can also add numbers at the end e.g $K_v3.1$ where the first number represents the gene subfamily and the second the specific channel isoform.

This scheme has a functional relevance.

2.3 Experimental techniques

2.3.1 Single channel recordings

Patch clamp technique: A glass electrode with a tip of less than 5 microm in diameter has been placed on the surface of a cell and suck a small part of the cell into the pipette. The rim of the pipette form a very high resistance seal, forcing most of the current to flow through the pipette. This gives much less noisy recordings because the outside of the patch we are measuring are practically isolated. With this technique they are able to measure the opening and closing of a single channel. The opening and closing of a single channel appears to be random, but we can see order in the statistics.

2.3.2 Channel isolation by blockers

A way of isolating different currents is by using channel blockers. E.g we can use tetrodotoxin from blowfish to block the Na^+ channels involved in generating action potentials.

2.3.3 Channel isolation by mRNA transfection

Inserting cDNA or mRNA of a protein in a cell which does not normally express that protein. This can form new types of channels in the cell? And we want for some reason to study the channels in the new environment?

2.3.4 Gating current

The movement of gating charges in the protein subunit is called the gating current or I_g . These currents tend to be much smaller than the ionic currents flowing through the membrane, so in order to measure I_g we need to reduce the ionic current, which can be done by replacing permeant ions with

impermeant ones or by using channel blockers. The gating current is outward. Gating currents are a useful tool for the development of kinetic models of channel activation.

2.4 Modelling ensembles of voltage-gated ion channels

2.4.1 Gating particle models

A type: (What is this?) Used when gene combination not known? Gives rise to action potentials that are delayed compared to the pure HH-model. This is because the A-type potassium channel is open as the membrane potential increases towards the spiking threshold, slowing the rise of the membrane potential. Eventually the A-type current inactivates, and the cell can spike.
 I_A

2.4.2 Thermodynamic models

In thermodynamic models the rate coefficients are given by functions derived from the transition state theory of chemical reactions (What is this?)
 For a gating particle represented by a gating variable x , the steady state activation is given by the sigmoid curve:

$$x_{\infty} = \frac{1}{1 + \exp(-(V - V_{1/2})/\sigma)}$$

where $V_{1/2}$ is the half activation voltage and σ is the inverse slope. The corresponding time constant is:

$$\tau_x = \frac{1}{\alpha'(V) + \beta'(V)} + \tau_0$$

where τ_0 is a rate-limiting factor

3 Exam questions

3.1 Electrical properties of neurons

1. What is the neuronal membrane made of

The bulk of the membrane is composed of a 5nm thick lipid bilayer; Two layers of lipids which have their hydrophilic ends pointed outwards and their hydrophobic ends pointed inwards.

2. How thick is the neuronal membrane?

About 5 nm

3. What is meant by the resting membrane potential?

The weighted average of the equilibrium potential of all the ions. K^+ higher concentration inside and diffuses easily through channels. The more K^+ that goes outside membrane, the more negative the inside becomes, and the electrical potential increases until it is big enough to counter the diffusion. Na^+ has both concentration gradient and electrical gradient going inwards, but the channels are not as eager to let them through

4. How big is typically the resting membrane potential?

Around -60mV

5. What are the key ions setting up the neuronal membrane potential and mediating electrical signals?

$Na^+, Ca^{2+}, K^+, Cl^-, OA^-$

6. What is an ion channel?

Ion channels are pores in the lipid bilayer, made of proteins, which can allow certain ions to flow through the membrane. The membrane

separates the extracellular fluid from the cytoplasm. To let certain ions through the membrane have several ion channels, which can be leak channels; always open, but may only accept certain types of ions. They can be pumps, which f.eks pump out 3 Na⁺ ions in exchange for 2 K⁺ ions with the use of one ATP molecule. We also have the active channels which are gated either by voltage or by ligands. Neurotransmitter receptors may be ligand gated. The channels in the axons is mostly voltage gated, which help create the action potential.

7. What are the two main categories of ion channels?

Active and passive channels

8. What is meant by an active channel?

An active channel can exist in open or closed states, depending on e.g membrane potential, ionic concentrations or the presence of bound ligands, such as neurotransmitters.

9. What is meant by a passive channel?

A passive channel does not change their permeability in responses to external influences

10. What is an ion pump?

An ion pump is an ion channel that pumps the ions in the "opposite direction" of where it want to go.

11. Which ion pump is particularly important for setting up the resting membrane potential?

When Na⁺ and K⁺ reaches equilibrium, there is no net flow of charge across the membrane, but there is net flow of Na⁺ and K⁺ and over time this would cause the concentration gradient to run down.

12. What is an electrogenic pump?

The Na⁺K⁺ pump is electrogenic, because it changes the net charge in the cell by pumping out more positive particles than it pumps in. It seems like if the pump uses ATP this is a good indication of it being electrogenic.

13. Describe the Nernst-Planck equation. What does it tell?

This equation is a general description of how charged ions move in solution in electric fields. (Where they are influenced by electrical drift and diffusion)

14. What is the Nernst potential?

This is the equilibrium potential for one permeable ion.

$$E_X = \frac{RT}{z_X F} \ln \frac{[X]_{out}}{[X]_{in}}$$

where $[X]_{out}$ and $[X]_{in}$ is their intracellular and extracellular concentrations of X

15. Derive the Nernst potential from the Nernst-Planck equation.

Concentration gradient:

$$J_{X,diff} = -D_X \frac{d[X]}{dx}$$

Where D_X is the diffusion coefficient of molecule X

Electrical drift:

$$J_{X,drift} = -\frac{D_X F}{RT} z_X [X] \frac{dV}{dx}$$

Where z_X is the ion's signed valency (the charge of the ion measured

as a multiple of the elementary charge). R is the gas constant, T is the temperature in kelvins and F is faradays constant.

Nerst-Planck:

$$J_X = -D_X \frac{d[X]}{dx} - \frac{D_X F}{RT} z_X [X] \frac{dV}{dx}$$

The Nernst equation is derived by assuming diffusion in one dimension along a line that starts at $x = 0$ and ends at $x = X$. For there to be no flow of current (which is what the Nernst equation describes) the Nernst planck equation must be zero.

$$\begin{aligned} \frac{1}{[X]} \frac{d[X]}{dx} &= - \frac{z_X F}{RT} \frac{dV}{dx} \\ \int_{E_m}^0 -dV &= \int_{[X]_{in}}^{[X]_{out}} \frac{RT}{z_X F [X]} \\ E_m &= \frac{RT}{z_X F} \ln \frac{[X]_{out}}{[X]_{in}} \end{aligned}$$

16. What is meant by the principle of electroneutrality?

each atom in a stable substance has a charge close to zero

17. Is a large deviation from electroneutrality needed to set up the resting membrane potential?

From direct measurements the specific membrane capacitance is often set to be $1 \mu F cm^{-2} = 10^{-8} \mu F \mu m^{-2}$

If we consider the squid giant axon with diameter $500 \mu m$ and a section $1 \mu m$ long, with resting potential $-70 mV$, we have Area: $500 \times 1 \times \pi \mu m^2$

C: $500\pi \times 10^{-8} \mu F$

Charge: $q = CV = 500\pi \times 10^{-8} \mu F * 70 * 10^{-3} V = 35000\pi \times 10^{-11} \mu C$

Faradays constant: $F = 96485.3365C/mol$ is the electrical charge of one mol of elektrons

Dividing by faradays: ...

volume: $\pi(500/2)^2\mu m^3$ change to liters and multiply by 400 mM per liter. We get that there is almost 10 million times as many ions in the cytoplasm than on the membrane, and the effect of charging the membrane (releasing 1 part in 10 million, does not really matter. So we can assume electroneutrality. This ofcourse is different for a very small neuron.

18. What does the Goldman-Hodgkin-Katz (GHK) model tell you?

GHK predict the current I_X mediated by a single ionic species X flowing across a membrane when the membrane potential is V.

19. What approximations are assumed in the GHK model?

- No current flows when the voltage is equal to the equilibrium potential. Electrical drift and diffusion is equal
- the current changes direction at the equilibrium potential.
- The individual ions do not obey ohm's law since the current is not proportional to the voltage.
- The potassium characteristic favours outward rectifying currents and the calcium characteristic favours inward rectifying currents.

20. The GHK model can account for inward and outward rectification of ion currents. What is meant by this?

Rectification is the property of allowing current to flow more freely in one direction than another. Potassium favours outward current, and is described as outward rectifying. Calcium favours inward currents and is described as inward rectifying.

21. In modeling one often assumes a quasi-ohmic relation between membrane potential and ion current. What is meant by quasi-ohmic?

Making a linear approximation to the GHK equations is similar to assuming ohm's law. Since the straight line does not necessarily pass through the origin, the correspondence is not exact and this form of linear I-V relation is called quasi-ohmic.

22. What is the capacitive current?

Capacitive current is the description of how current affects the voltage across the membrane

23. Derive/show a mathematical expression for it.

Capacitance is defined as $q = CV$. The current flow through the membrane is $I = \frac{dq}{dt}$

We can differentiate:

$$I = \frac{dq}{dt} = C \frac{dV}{dt}$$

The change in voltage over time, during the charging or discharging of the membrane, is inversely proportional to the capacitance.

24. Derive a general expression for the reversal potential (E_m) for a neuron with several quasi-ohmic ion channels.

????

25. Derive a differential equation for a simple RC-circuit neuron.

??

26. Show that the solution for the membrane potential V for this RC-circuit neuron receiving a constant step current at time $t = 0$ is given by $V(t) = A + B(1 - \exp(-t/C))$. Determine the constants A , B , and C .

??

27. What is the limiting value of V when $t \rightarrow \infty$

..

28. At time t_e the current is turned off. Show that the solution for the membrane potential V for the RC-circuit neuron receiving after time t_e is given by $V(t) = A' + B' \exp(-(t - t_e)/C')$. Determine the constants A' , B' , and C' .

..

29. What is the membrane time constant τ_m ?

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30. What is the input resistance?

Input resistance is defined as the change in the steady state membrane potential divided by the injected current causing it. To determine the input resistance, the resting membrane potential is first measured. Then a small amount of current I_e is injected and the membrane potential is allowed to reach a steady state V_∞ . The input resistance is then given by.

$$R_{in} = \frac{V_\infty - E_m}{I_e}$$

3.2 Hodgkin-Huxley model

1. Why was Hodgkin and Huxley's development of their model of action potential propagation so important?

It was used to calculate the form of the action potentials in the squid giant axon. Their work was the starting point for the biophysical understanding of the structures now known as ion channels

2. Why did they focus on the squid giant axon?

Because it is giant. The large diameter allowed them to insert voltage clamps.

3. Outline the scientific approach Hodgkin and Huxley used to develop their model.

- Voltage clamp experiments are done to determine the kinetics of a particular type of channel. Nowadays the methods of recording and isolating currents through particular channel types are more advanced.
- A model of a channel type is constructed by fitting equations, often of the same mathematical form, to the recordings.
- Models of axons, dendrites or entire neurons are constructed by incorporating models of individual channel types in the compartmental models. Once the equations for the models are solved, action potentials and other behaviours of the membrane potential can be simulated.

4. What is meant by current clamp?

Voltage clamp: Injects current to hold the membrane potential constant at desired value

Current clamp: injects current to deliberately change the membrane potential, to f.eks trigger an action potential.

5. What is meant by space clamp?

Electrodes are long, thin wires that short circuit the electrical resistance of the cytoplasm and the extracellular space. This ensures that the potential is uniform over a large region of membrane and that therefor there is no axial current in the region. In this configuration the membrane current is identical to the electrode current, so the membrane current can be measured exactly as the amount of electrode current to be supplied to keep the membrane at the desired value. when the voltage clamp is used to set the membrane potential to a constant value $\frac{dV}{dt} = 0$ which means the voltage clamp current is equal to the ionic current.

6. What ion channel currents were included in the model?

Sodium current, potassium current, and leak current, which is mostly made up of chloride ions. The potassium and Sodium channels are active channels.

7. Outline the model for the potassium current?

$$I = I_c + I_i = C_m \frac{dV}{dt} + I_i$$

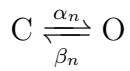
$$I_i = I_{Na} + I_K + I_L = g_{Na}(V - E_{Na}) + g_K(V - E_K) + \bar{g}_L(V - E_L)$$

8. What is a gating particle?

HH-model: The membrane contains gates, which are guarded by a number of independent gating particles, which controls if the permeable ion can pass or not

9. How is the dynamics of the gating particles modeled in the Hodgkin-Huxley model?

The movement of a gating particle between its closed(C) and open (O) positions can be expressed as a reversible chemical reaction:



The fraction of gating particles in an open state is n , the fraction in closed state is $1 - n$

There is a rate law corresponding to the equation above:

$$\frac{dn}{dt} = \alpha_n(1 - n) - \beta_n n$$

Solving this gives:

$$n(t) = n_\infty(V_1) - (n_\infty(V_1) - n_0) \exp(-t/\tau_n(V_1))$$

$$n_\infty = \frac{\alpha_n}{\alpha_n + \beta_n}$$

$$\tau_n = \frac{1}{\alpha_n + \beta_n}$$

Where n_∞ is the limiting probability of a gating particle being open if the membrane potential is steady as t approaches infinity and τ_n is a time constant

$$\frac{dn}{dt} = \frac{n_\infty - n}{\tau_n}$$

10. How were the model parameters describing the potassium current determined?

$$n_{\infty} = \left(\frac{g_{k\infty}}{\bar{g}_k} \right)^{1/4}$$

Finding 11. Outline the model for the sodium current?

12. How does the model for the sodium current differ from the model for the potassium current?
13. What is an inactivation variable?
14. What ions carry the leak current?
15. What is an absolute refractory period?
16. What is a relative refractory period?
17. How does the Hodgkin-Huxley model account for the refractory period of neurons?
18. How does the ion-channel dynamics typically depend on temperature?
19. What is a Q10 factor?

4 Multicompartmental modelling and cable equation

1. What does it mean when a neuron is said to be isopotential?

An area where the membrane potential is effectively constant.

2. Is "isopotentiality" always a good approximation?

Nah, most neurons cannot be considered isopotential throughout, which leads to axial current flowing along the neurites. F.eks during an action potential

different part of the axon are at different potentials.

3. How can non-isopotential neurons be modeled?

Compartment model, cable equation

4. Describe the principles behind multicompartmental modeling.

Split up the neurite into cylindrical compartments. Area of compartment: $a = \pi dl$. Because the intracellular resistance is much greater than the extracellular resistance, it may be acceptable to consider the extracellular component to be effectively zero. We then model the extracellular medium as electrical ground

The axial resistance of a compartment is proportional to length l and inversely proportional to the cylinder's cross-section area $\frac{\pi d^2}{4}$

The axial resistivity, also known as the specific axial resistance R_a is $4R_a l / \pi d^2$

$$I_{c,j}a + I_{i,j} = I_ja + I_{e,j}$$

Injected current is actually current. All the other currents are actually current densities and must be multiplied by the area to become a current.

$$I_ja = \frac{V_{j+1} - V_j}{4R_a l / \pi d^2} + \frac{V_{j-1} - V_j}{4R_a l / \pi d^2}$$

R_a is a resistivity, not a resistance as it may look like. To get resistance we use $R = \rho L / A$ where ρ is resistivity and A is the cylinder cross sectional area. Hva i alle dager skjer med enhetene? 5. What is meant by killed(open)-end, sealed-end and leaky-end boundary conditions?

Killed end: The end of the neurite has been cut, which means that the membrane potential at the end of the neurite is equal to the extracellular potential

and $V_0 = 0$

Sealed end: Tip of neurite very small, resistance very high. The gradient of the membrane potential along the neurite is proportional to the axial current. Zero current flowing through the end implies that the gradient of the membrane potential at the end is zero: $V_1 = V_{-1}$ from midpoint definition of the derivative.

Leaky end: resistance at the end of the cable has a finite absolute value R_L . The boundary condition is derived by equating the axial current, which depends on the spatial gradient of the membrane potential, to the current flowing through the end $(V - E_m)/R_L$

6. Derive the cable equation from the fundamental equation for multicompartmental modeling.

Just make the compartments small. Gives pde 7. Derive the steady-state solution for a semi-infinite cable with a constant current injected in one end.

?? 8. What is the length constant λ ?

It determines the shape of the exponential voltage decay along the length of the cable. It is determined by the specific membrane resistance, the axial resistivity and the diameter of the cable

9. What is the input resistance for a semi-infinite cable with a constant current injected in one end?

??

5 Synapses

1. What is a synapse?

The chemical synapse is a complex signal transduction device that produces

a postsynaptic response when an action potential arrives at the presynaptic terminal 2. What are the two main types of synapses?

Electrical or chemical?

Inhibitory or excitatory

3. Describe some common postsynaptic receptors.

Ionotropic receptors are linked directly to ion channels (the Greek *tropos* means to move in response to a stimulus). These receptors contain two functional domains: an extracellular site that binds neurotransmitters, and a membrane-spanning domain that forms an ion channel (Figure 7.9A). Thus ionotropic receptors combine transmitter-binding and channel functions into a single molecular entity (they are also called ligand-gated ion channels to reflect this concatenation). Such receptors are multimers made up of at least four or five individual protein subunits, each of which contributes to the pore of the ion channel.

The second family of neurotransmitter receptors are the metabotropic receptors, so called because the eventual movement of ions through a channel depends on one or more metabolic steps. These receptors do not have ion channels as part of their structure; instead, they affect channels by the activation of intermediate molecules called G-proteins (Figure 7.9B).

In neuroscience, synaptic plasticity is the ability of synapses to strengthen or weaken over time, in response to increases or decreases in their activity

4. Describe how the electrical response at the postsynaptic side of a chemical synapse can be modulated.

5. Describe various mathematical functions used to model the postsynaptic conductance following the presynaptic arrival of an action potential.

6. What is meant by synaptic plasticity?

In neuroscience, synaptic plasticity is the ability of synapses to strengthen or weaken over time, in response to increases or decreases in their activity

The response of one spike depend on the response of another

7. What is synaptic depression?

8. What is synaptic facilitation?

9. What is long-term potentiation (LTP)?

10. What is spike-timing dependent plasticity?

11. How are electrical synapses modeled?

Ohmic connection

6 Active ion channels

1. What distinguishes active and passive ion channels? Passive ion channels are always open to certain ions, and active channels are only opened by certain changes in the membrane or cellular fluids

2. What is meant by voltage-gated ion channels? Voltage gated ion channels

resonds to changes in the membrane potential

3. What is meant by ligand-gated ion channels?

Ligands are molecules specific for a reseptor. The ligand-gated ion channels have reseptors that respond to the presence of certain ligands.

4. Describe the structure of a voltage-gated ion channel.

5. Approximately how many voltage-gated ion channel types exist in humans?

143 6. Describe three nomenclature (naming) schemes for ion channels.

IUPHAR

Gene

Ad hoc

7. Mention and four experimental techniques for investigating ion channels.

Channel blockers

Patch clamp technique/gigaseal

8. Describe the structure of gating-particle models for ion channel currents.

7 Intracellular signaling and calcium

1. Why do neuroscientists often model the concentration of calcium (but not so often the concentration of sodium, potassium and chloride)?

Sodium potassium concentration is fairly constant. Ca is not. In addition Ca plays a major role in a multitude of intracellular signalling pathways.

2. Describe the diffusion equation.

$$\frac{\partial c}{\partial t} = D \left(\frac{\partial^2 c}{\partial x^2} + \frac{\partial^2 c}{\partial y^2} + \frac{\partial^2 c}{\partial z^2} \right) = D \nabla^2 c$$

3. Why is diffusion important for describing ion transport inside neurons (but less so for transport of signals/molecules between different cortical areas)?

4. Set up a differential equation for the dynamics of calcium concentration and describe various fluxes that in general contribute to this dynamics. Also, briefly describe the mathematical formulas describing the various calcium flux contributions.

8 Simplified neuron models

1. Why is it desirable to make “simplified” neuron models?

- We wish to explain how a complicated neural model works by stripping it down to its bare essentials. This gives an explanatory model in which the core mechanisms have been exposed and so are easier to understand
- We wish to understand the behaviour of a network descriptive model of

a neuron that describes the essential function of the neurons in question, an which is faster to simulate than compartmental neurons or which allows mathematical analysis of the network.

2. Why does one typically skip the modeling of spike propagation down the axon in network simulations?

We generate and receive firing rates rather than spike times. These models are appropriate for applications in which precise firing times are not very important to the network behavior

3. What is a two-compartment model?

A model only using two compartments. For example one dendrite compartment and one soma compartment

4. The Morris-Lecar for spike generation model has only two dynamical variables while the Hodgkin-Huxley model has four. What is the main advantage of being able to study a two-dimensional dynamic model instead of a four-dimensional one?

It reduces computational time.

Two dynamic variables allows for phase-plane analysis (appendix B.2)

5. What is an integrate-and-fire neuron?

Early HH-model

RC circuit used to model the passive patch of membrane with a spike generation and reset mechanism added. RC circuit gets a switch over resistance, which closes when the membrane potential reaches a specified threshold level.

6. What is the equation for the subthreshold membrane dynamics in the integrate-and-fire model?

$C_m \frac{dV}{dt} = -\frac{V-E_m}{R_m} + I$ C is membrane capacitance, R is membrane resistance

and I is the total current flowing into the cell, which would come from an electrode or from synapses.

7. How is spiking, i.e., firing of an action potential, achieved in the model? When the membrane reaches the threshold θ , the neuron fires a spike and the membrane potential V is reset to E_m . We can solve the equation for subthreshold voltage with small currents and get:

$$V = E_m + R_m I (1 - \exp(-t/\tau_m))$$

If $R_m I$ is bigger than the threshold θ , the voltage will cross the threshold at some point in time. The membrane potential then resets to zero and the process repeats. 8. Derive an expression for the f-I curve for an integrate-and-fire neuron with an absolute refractory period.

For a given level of current injection starting at time $t = 0$, at the time T_s a spike occurs, when the membrane potential is equal to θ . By substituting $V - E_m = \theta$ and $t = T_s$ and rearrange.

$$\theta = E_m + R_m I (1 - \exp(-T_s/\tau_m))$$

If we omit the leak current, we do not change the dynamics, the resting potential E_m is set to 0 mV.

Solve for T_s

The interval between consecutive spikes during constant current injection is the sum of the time to spike and the absolute refractory period $T_{interval} = T_s + \tau_r$ and the spike frequency $f(I) = \frac{1}{\tau_r + T_s}$. 9. What is a conductance-based synapse?

We describe a synaptic input using the conductance

$$g_{syn} = \bar{g}_{syn} \exp\left(-\frac{t - t_s}{\tau_{syn}}\right) H(t - t_s)$$

$$I_{syn}(t) = g_{syn}(t)(V(t) - E_{syn})$$

Where E_{syn} is the reversal potential for the synapse under consideration. This can be included in an integrate-and-fire neuron by including the current in the total current. 10. What is a current-based synapse?

To make the model easier to analyse and faster to simulate we can use the time course of the synaptic current, rather than the conductance.

$$I_{syn}(t) = I_{syn}^- \exp\left(-\frac{t - t_s}{\tau_{syn}}\right) H(t - t_s)$$

There is no dependence of the current on the membrane potential. For typical excitatory synapses, current-based synapses provide a reasonable approximation to conductance-based synapses. Implicit is that I_{syn}^- is the product of \bar{g}_{syn} and a constant driving force 11. Why is a current-based synapse a good approximation for AMPA receptors, but maybe less so for GABA receptors? E_{syn} for AMPA is ≈ 0 mV, which means $V - E_{syn}$ is almost constant. E_{syn} for GABA is typically close to E_m (slightly more hyperpolarized), so not so constant.

12. What is a Poissonian spike train?

The probability of firing an action potential per time unit is constant

Characterized by decaying interspike interval distribution 13. What is the interspike interval distribution for Poissonian spike train?

????????????

A decaying exponential function

14. Does cortical neurons exhibit such interspike interval distributions?

???????

Yes.

15. What is meant by balanced excitation and inhibition?

It means the total input from excitatory and inhibitory synapses are equal. That is, the magnitude of the input times the number of inputs is equal between the two.

16. What is the Stein model?

Integrate-and-fire neuron receiving infinitely short current pulses (δ -function pulses) with Poisson distribution from a number of excitatory and inhibitory neurons, causing the membrane potential to fluctuate and sometimes cross the threshold.

17. How can the standard integrate-and-firing neuron be modified to exhibit spike-rate adaptation?

We can add a current with a conductance that depends on the neuronal spiking. Whenever the neuron spikes, the adaptive conductance g_{adapt} is incremented by an amount Δg_{adapt} and otherwise it decays with a time constant of τ_{adapt} :

$$\frac{dg_{adapt}}{dt} = -\frac{g_{adapt}}{\tau_{adapt}}$$

18. What is the quadratic integrate-and-fire model (QIF)?

It replaces the $(V - E_m)/R_m$ term in the integrate-and-fire neuron

$$C_m \frac{dV}{dt} = -\frac{(V - E_m)(V_{thresh} - V)}{R_m(V_{thresh} - E_m)} + I$$

19. What is the exponential integrate-and-fire model (EIF)?

$$C_m \frac{dV}{dt} = -\left(\frac{V - E_m}{R_m} - \frac{\Delta_T}{R_m} \left(\frac{V - V_T}{\Delta_T}\right)\right) + I$$

Where V_T is a threshold voltage and Δ_T is a spike slope factor that determines the sharpness of spike initiation.

It is asymmetrical in comparison to the QIF

20. How may noise change the dynamics of integrate-and-fire neurons?

The noise allow the neuron to fire even when the mean input $I(t)$ would not be enough to cause a deterministic neuron with the same threshold to fire.

21. How can noise be added to the integrate-and-fire model?

We can model it by diffusive noise by adding a stochastic term to the membrane equation. We can add $\sigma \Delta W(t)$ to an euler equation, where ΔW is a random variable drawn from a Gaussian distribution with a mean of zero and a variance of Δt ; σ parameterizes the level of noise.

An alternative is to have a noisy threshold.

22. What is meant by a firing rate?

- The average firing rate of a single neuron determines by counting the spikes in a time window (often averaged over many presentations of a stimulus)
- The population firing rate (averaged over many neuron over one instance in time).

A firing rate function $f(I)$ tells what steady-state firing rate is obtained with constant input current I

23. Explain the difference between the stimulus-averaged firing rate and

the population firing rate?

See 22

24. What is the firing-rate function $f(I)$?

See 22.

25. Describe various mathematical functions used to model the firing-rate function?

$f = kl$ for $I > \theta$ 0 else

$f(I) = \frac{\bar{f}}{1 + \exp(-k(I - \theta))}$ where \bar{f} is the maximum firing rate, θ is the threshold and k controls the slope of the f - I curve. For large values of k , the sigmoid curve approximates to a step function.

$f = H(I - \theta)$

The heaviside example is sometimes referred to as McCulloch-Pitts neurons.

26. What is meant by a feed forward network?

The synaptic current in an output neuron is derived from the firing rates of the input neurons to which it is connected and the appropriate synaptic conductances; there are no loops which allow feedback.

If each input neuron, labelled with the subscript i , fires at a constant rate, the current flowing into an output cell, labelled j , will also be constant:

$$I_j = \sum w_{ij} f_i \quad f_i = f(I_i)$$

27. What is meant by a recurrent network?

A network similar to the feed forward, but now we also have some feedback creating loops

28. What is a dynamic firing-rate model? If the inputs to the network vary in time

??

$$\tau_{syn} \frac{dI_i}{dt} = -I_i + \sum w_{ij}$$

1. Mention some experimental techniques that is used to measure cortical activity.

Finne ut mer

2. What is meant by "physics-type" multimodal modelling?

Finne ut mer

3. Describe the principles of measuring extracellular potentials in the brain.

LFP inside cortex

ECoG outside cortex

EEG on scalp

Two electrodes and measures potential difference.

4. What is meant by (i) LFP, (ii) MUA, (iii) ECoG, (iv) EEG?

LFP - Local field potential, low pass filter, measure dendritic processing of synaptic input.

MUA - Multi-unit activity, high pass filter, measure of neuronal action potentials

ECoG - Measures from surface of brain

EEG - Measures from the scalp

5. Describe volume conductor theory and its underlying assumptions.

Visualizes brain tissue as two domains: a continuous extracellular domain and

a non continuous intracellular domain

Neuron is two compartments

Densiritten er en source, soma en sink

Beskriver EC med konduktiviteten σ

6. Derive an equation for the extracellular potential set up by a point current source.

$$-j = \sigma E$$

7. Why cannot point-neuron models (alone) be used to compute extracellular potentials?

Then we get zero potential. Just as much current goes in as out.

8. What is the simplest neuron model that can be used to compute extracellular potentials?

Two compartment model

9. What is the formula for the extracellular potential set up by a two-compartment neuron model?

$$\phi(r, t) = \frac{1}{4\pi\sigma} \left(\frac{I(t)}{|r - r_1|} - \frac{I(t)}{|r - r_2|} \right)$$

10. Sketch the LFP set up by a two-compartment neuron model receiving a single excitatory synaptic input in (i) the soma compartment og (ii) the dendrite compartment.

11. What is the formula for the extracellular potential set up by a general multicompartment neuron model with N compartments?

