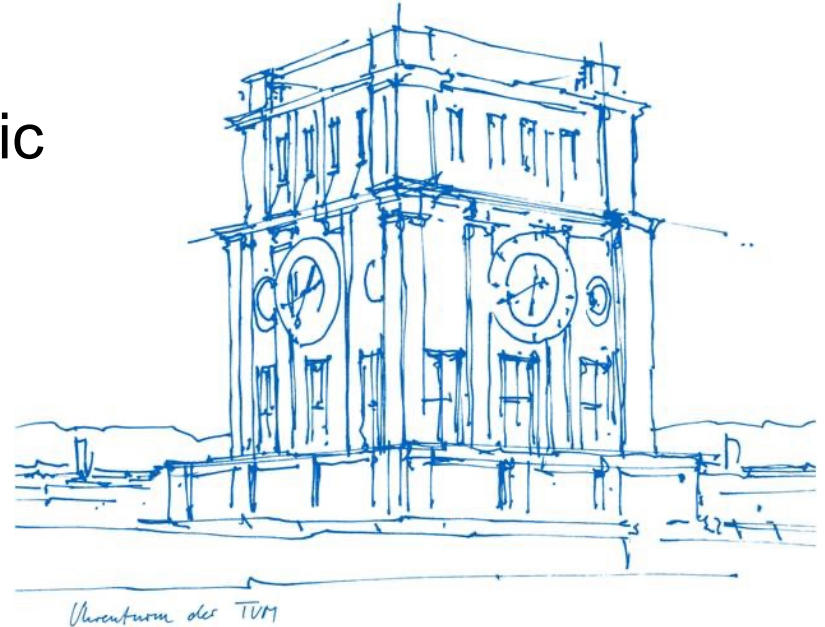


Seminar: Computational Methods for Image Reconstruction

Chapter 3: Analytical Tomographic Image Reconstruction Methods:

Wise 2023/24

Presenter: Boey Kai Zhe



Topics

Introduction

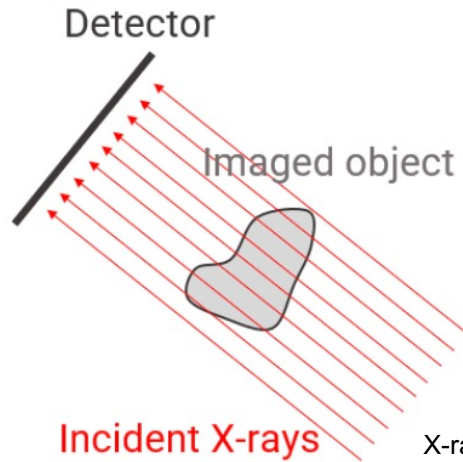
2D fan beam tomography

3D cone-beam reconstruction

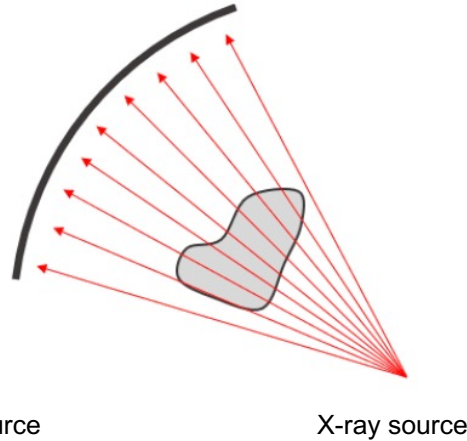
Outlook on advanced methods

Conclusion

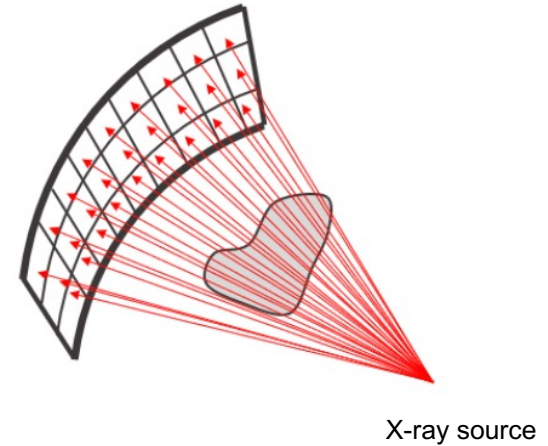
X-ray CT Geometries



Parallel beam



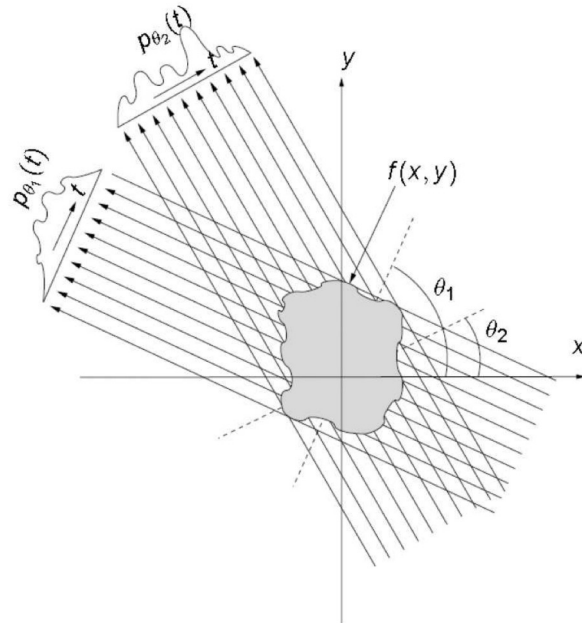
Fan beam



Cone beam

Image: <https://imaging.rigaku.com/blog/how-does-ct-reconstruction-work>

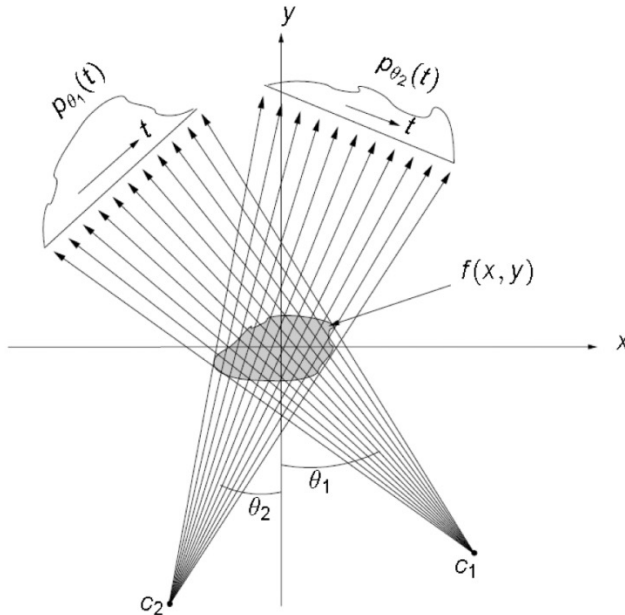
Parallel Beam Geometry



- 1st Generation CT
- Year developed: 1971
- Anatomy: Head only
- Principle: Translate – Rotate (Pencil beams were translated to cover the object from each view and then rotated)
- Time to acquire 1 image: ~5 min
- Slow, not practical!!

Image: <https://www5.cs.fau.de/fileadmin/lectures/2017w/Lecture.2017w.ProjFCR/fanBeamRecon.pdf>

Fan Beam Geometry (Topic of presentation)



- 3rd Generation CT
- Year developed: 1975
- Anatomy: All anatomy
- Principle: Rotate – Rotate (source and detector rotated together)
- Time to acquire 1 image: 1 sec
- Fast, widely use today.

Image: <https://www5.cs.fau.de/fileadmin/lectures/2017w/Lecture.2017w.ProjFCR/fanBeamRecon.pdf>

Cone Beam Geometry (Topic of presentation)

- Very similar in geometry to fan beam CT.
- Difference in the detector where it has more rows.
- Even fewer rotations needed than fan-beam

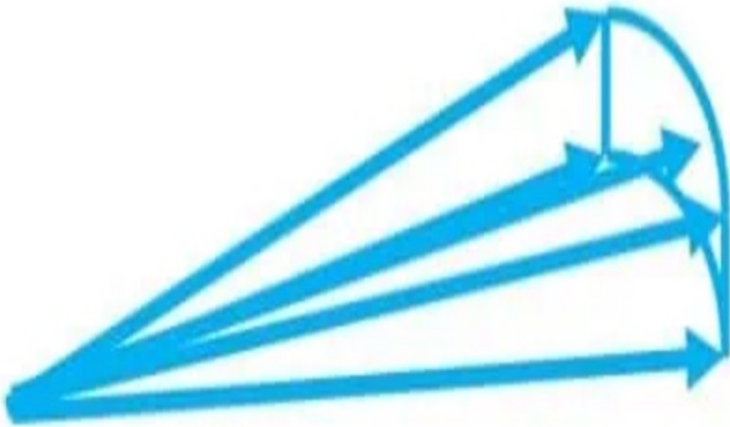


Image: <https://www5.cs.fau.de/fileadmin/lectures/2017w/Lecture.2017w.ProjFCR/fanBeamRecon.pdf>

Topics

Introduction

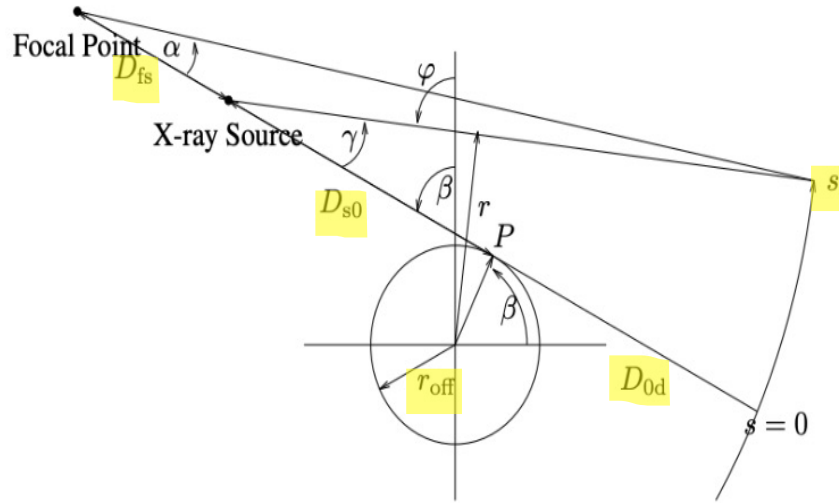
2D fan beam tomography

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Outlook on advanced methods

Conclusion

Properties of Fan Beam Geometry



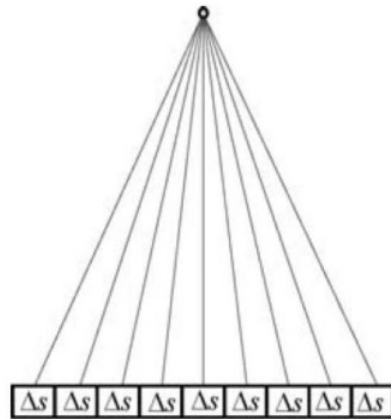
Distance parameters

- D_{fs} - the distance from the focal point f to the X-ray source s ;
- D_{s0} - distance from the X-ray source s to P
- D_{0d} - distance from p to the center of detector d
- $D_{sd} = D_{0d} + D_{s0}$ (total distance from the X-ray source to the center of the detector)
- $s \in [-s_{max}, s_{max}]$ - arc length along the detector
- r_{off} - mismatch distance between isocenter and D_{sd}

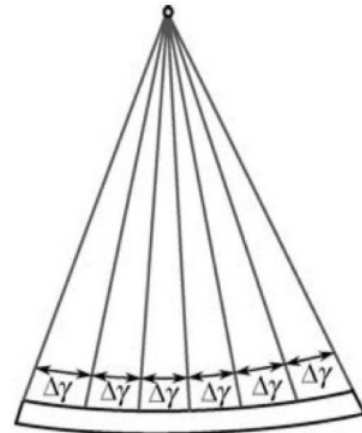
Image: J. Fessler. Image reconstruction: Algorithms and analysis. [5]

2 Cases of Fan Beam Geometry

Image: <https://www5.cs.fau.de/fileadmin/lectures/2017w/Lecture.2017w.ProjFCR/fanBeamRecon.pdf>



Flat-Detector Fan-Beam



Curved-Detector Fan-Beam

Equidistant case

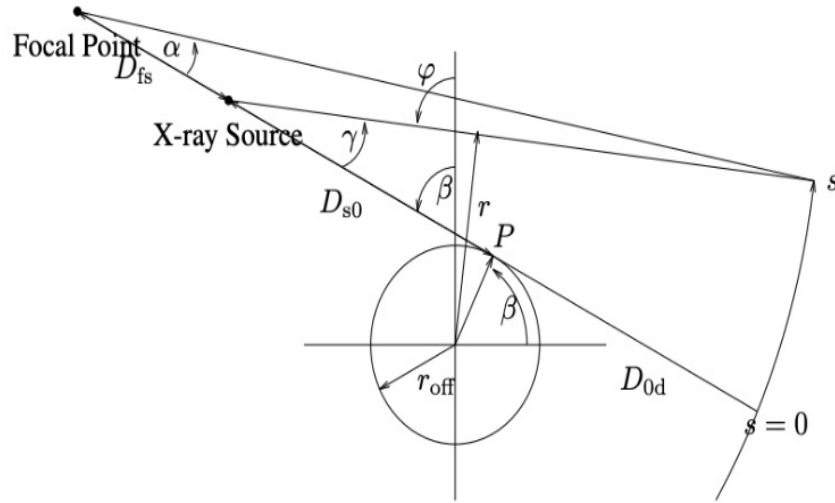
- Flat detector
- $D_{fs} = \infty$

Equiangular case

- Curve detector
- $D_{fs} = 0$

Image: Zeng, 2009 [4]

Properties of Fan Beam Geometry (Continue)



Angular parameters

- β - angle that the line segment between the X-ray source and the detector center makes with the y axis.

$$\gamma(s) = \begin{cases} \frac{s}{D_{sd}}, & \text{if } D_{fs} = 0 \text{ (equiangular)} \\ \arctan(\frac{s}{D_{sd}}), & \text{if } D_{fs} = \infty \text{ (equidistant)} \end{cases} \quad (1)$$

$$s(\gamma) = \gamma^{-1}(s) = \begin{cases} D_{sd}\gamma, & \text{if } D_{fs} = 0 \text{ (equiangular)} \\ D_{fd}[\gamma - \arcsin(\frac{D_{fs}}{D_{fd}} \sin \gamma)], & \text{if } 0 \leq D_{fs} \leq \infty \\ D_{sd} \tan \gamma, & \text{if } D_{fs} = \infty \text{ (equidistant)} \end{cases} \quad (2)$$

Image: J. Fessler. Image reconstruction: Algorithms and analysis. [5]

Forward projection

More definitions:

- $L(s, \beta) = \{(x, y) : x \cos \phi(s, \beta) + y \sin \phi(s, \beta) = r(s)\}$ - the ray corresponding to angle β and detector element s ;
- $\gamma_{max} = \gamma(s_{max})$ and s_{max} is **half** of the total arc length of the detector.
- r_{max} - field of view
- $2\gamma_{max}$ - fan angle
- $|r(s)| \leq r_{max} = D \sin \gamma_{max}$

With some derivations, we obtain the forward projection:

$$p(s, \beta) = \int_{L(s, \beta)} f(x, y) \, d\ell = \iint f(x, y) \delta(x \cos \phi(s, \beta) + y \sin \phi(s, \beta) - r(s)) \, dx \, dy \quad (3)$$

Goal: reconstruct $f(x, y)$ by estimating its absorption coefficient

Filter-backproject (FBP) for 360° scan

Simple derivation:

- Begin with the definition of the Parallel-beam fbp:

$$f(x, y) = \frac{1}{2} \int_0^{2\pi} \int p_\phi(r) h_*(x \cos \phi(s, \beta) + y \sin \phi(s, \beta) - r) dr d\phi \quad (5) \quad , \text{where } h_*(.) \text{ denotes the ramp filter}$$

- Change of variable $r=r(s)$ & $\phi = \phi(s, \beta)$, jacobian of the determinant: $J(s) \triangleq |D_{s0} \cos \gamma(s) - r_{\text{off}} \sin \gamma(s)| |\dot{\gamma}(s)|$.
- Applying change of variable to (5), we get:

$$f(x, y) = \frac{1}{2} \int_0^{2\pi} \int w_{2\pi}(x, y; \phi(s, \beta)) p(s, \beta) h_*(x \cos \phi(s, \beta) + y \sin \phi(s, \beta) - r(s)) J(s) ds d\beta \quad (6)$$

- Given $x_\beta = x \cos \beta + y \sin \beta$ and $y_\beta = -x \sin \beta + y \cos \beta$, using trigonometric identities, the following relationship are obtained:

Continuation:

$$L_{\beta}(x, y) = \sqrt{(D_{s0} - y_{\beta})^2 + (x_{\beta} - r_{\text{off}})^2} \quad (7)$$

$$\gamma_{\beta}(x, y) = \arctan \left(\frac{x_{\beta} - r_{\text{off}}}{D_{s0} - y_{\beta}} \right) \quad (8)$$

$$s_{\beta}(x, y) = \begin{cases} D_{sd} \gamma_{\beta}(x, y), & \text{if } D_{fs} = 0 \text{ (equiangular)} \\ D_{sd} \tan \gamma_{\beta}(x, y), & \text{if } D_{fs} = \infty \text{ (equidistant)} \end{cases} \quad (9)$$

- Substituting equation (7), (8) and (9) into (6) and applying some scaling property and algebraic manipulation, the formula for fan beam reconstruction can be simplified as:

$$f(x, y) = \int_0^{2\pi} \frac{1}{W_2^2(x, y, \beta) L_{\beta}^2(x, y)} \left[\int p(s, \beta) \frac{W_{2\pi(s, \beta)} J(s)}{W_1^2(s)} g_*(s_{\beta}(x, y) - s) ds \right] d\beta \quad \star \quad (10)$$

- W_1 and W_2 are some the weight function and $g_*(s)$ is the ramp filter, which are different for both equiangular and equidistant case.

Outline of the FBP formula

- Step 1: Compute weighted projections for each β

$$\bar{p}(s, \beta) = p(s, \beta) \frac{w_{2\pi}(s, \beta) J(s)}{W_1^2(s)} \quad (11)$$

- Step 2: Filter those weighted projections (along s) for each β using the modified ramp filter

$$\bar{p}(s, \beta) = \bar{p}(s, \beta) * g_s(s) \quad (12)$$

- Step 3: Perform a weighted backprojection of those filtered projections

$$f(x, y) = \int_0^{2\pi} \frac{1}{W_2^2(x, y, \beta) L_\beta^2(x, y)} \bar{p}(s_\beta(x, y), \beta) d\beta \quad (13)$$

Equiangular case/ curved detector

- Projection weighting ratio in equation (11)

$$\frac{J(s)}{W_1^2(s)} = J(s) = \frac{1}{D_{sd}} |D_{so} \cos \frac{s}{D_{sd}} - r_{off} \sin \frac{s}{D_{sd}}| \approx \frac{D_{so}}{D_{sd}} \cos \frac{s}{D_{sd}} \quad (15)$$

- Modified ramp filter in equation (12), where Δs denotes the detector element spacing:

$$h[n] = \begin{cases} \frac{1}{4\Delta_s^2}, & n = 0 \\ 0, & n \text{ even} \\ \frac{-1}{[\pi D_{sd} \sin(n\Delta_s/D_{sd})]^2}, & n \text{ odd} \end{cases} \quad (16)$$

- Backprojection weighting ratio in equation (13)

$$\frac{1}{W_2^2 L_\beta^2(x, y)} = \frac{D_{sd}^2}{L_\beta^2(x, y)} = \frac{D_{sd}^2}{(D_{so} - y_\beta)^2 + (x_\beta - r_{off})^2} \quad (17)$$

Equidistant case/ flat detector

- Projection weighting ratio in equation (11), reminder $\gamma(s) = \arctan(s/ D_{sd})$

$$w_{2\pi}(s, \beta) \frac{J(s)}{W_1^2(s)} = \frac{w_{2\pi}(s, \beta)}{D_{sd}} |D_{so} \cos \gamma(s) - r_{off} \sin \gamma(s)| \approx w_{2\pi}(s, \beta) \frac{D_{so}}{\sqrt{D_{sd}^2 + s^2}} \quad (19)$$

- Ordinary ramp filter in equation (12):

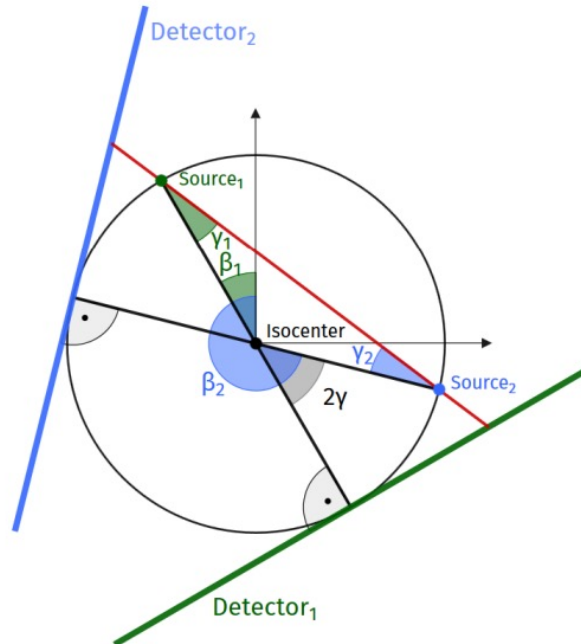
$$h[n] = \begin{cases} 1, & n = 0 \\ 0, & n \text{ even} \\ \frac{-1}{(\pi n/2)^2}, & n \text{ odd} \end{cases} \quad (20)$$

Demo !!

- Backprojection weighting ratio in equation (13)

$$\frac{1}{W_2^2 L_\beta^2(x, y)} = \frac{D_{sd}^2}{(\cos \gamma_\beta(x, y) L_\beta(x, y))^2} = \frac{D_{sd}^2}{(D_{so} - y_\beta)^2} \quad (21)$$

FBP for short scans (<360°)



- For a 360° rotation, every ray is sampled exactly twice.
- Given 2 identical rays (β_1, γ_1) and (β_2, γ_2) are identical:

$$\gamma_2 = -\gamma_1$$

$$\beta_2 = \beta_1 + 2\gamma_1 + \pi$$
- Short scan setting: $\beta_{max} = \pi + 2\gamma_{max}$, every point in the equivalent parallel-beam sinogram is sampled at least once.

Image: <https://www5.cs.fau.de/fileadmin/lectures/2017w/Lecture.2017w.ProjFCR/fanBeamRecon.pdf>

Solution: Parker's weighting

- Replace Parker's weighting with regular projection weighting in (11)
- Parker's weighting:

$$w_{2\pi}(s, \beta) = \begin{cases} q\left(\frac{\beta}{2(\gamma_{\max} - \gamma)}\right), & 0 \leq \beta \leq 2(\gamma_{\max} - \gamma) \\ 1, & 2(\gamma_{\max} - \gamma) < \beta < \pi - 2\gamma \\ q\left(\frac{\pi + 2\gamma_{\max} - \beta}{2(\gamma_{\max} + \gamma)}\right), & \pi - 2\gamma \leq \beta \leq \pi + 2\gamma_{\max} \end{cases} \quad (22)$$

→ Identical rays

- $q(x) = \sin^2\left(\frac{\pi}{2}x\right)$

Demo !!

Backproject-filter (BPF) approach

- Given fan-beam projection $p(s, \beta)$, $\beta \in [0, \beta_{max}]$, weighting function $w_{bpf}(s, \beta)$, the weighted backprojection

$$b(x, y) == \int_{-s_{max}}^{s_{max}} \int_0^{\beta_{max}} \delta(x \cos \phi(s, \beta) + y \sin \phi(s, \beta) - r(s)) w_{BPF}(s, \beta) ds d\beta \quad (23)$$

- Algorithm
 - Step 1. Backproject the projection measurements
 - Step 2. Take the two-dimensional FFT of the backprojection image.
 - Step 3. Apply the ramp filter to the Fourier transformed image.
 - Step 4. Take the inverse two-dimensional FFT of the filtered image to obtain the reconstruction

Demo !!

Fan-parallel rebinning

- Transform the fan-beam projections into parallel-beam projections by finding equal rays in both geometries
- Idea, express $p(s, \beta)$ in terms of parallel beam projections.
- How? Use change of variable (i) $\phi = \beta + \gamma$ and (ii) $r = D_{so} \sin \gamma$, we can write:

$$p_{\phi}(r) = p(s, \beta)|_{s=s(r), \beta=\beta(r, \phi)} = p(\gamma^{-1}(\arcsin r/D_{so}, \phi - \arcsin r/D_{so})) \quad (4)$$

- Perform 2 interpolation steps:
 - (i) angular interpolation - 1D interpolation along the source position using the relationship $\phi = \beta + \gamma$
 - (ii) radial interpolation - 1D interpolation along the detector using the relationship $r = D_{so} \sin \gamma$
- Inaccurate due to to interpolation, hence, choose FBP if possible

Demo !!

Topics

Introduction

2D fan beam tomography

3D cone-beam reconstruction

Outlook on advanced methods

Conclusion

Cone Beam Geometry

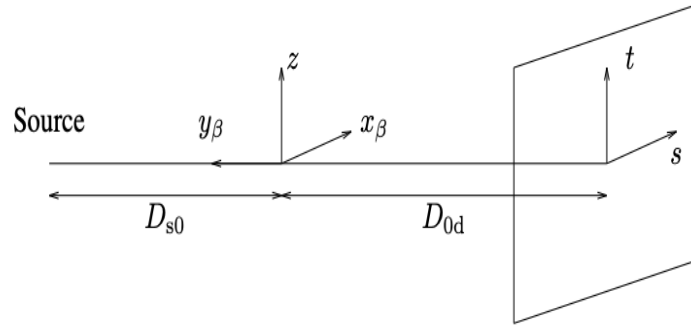
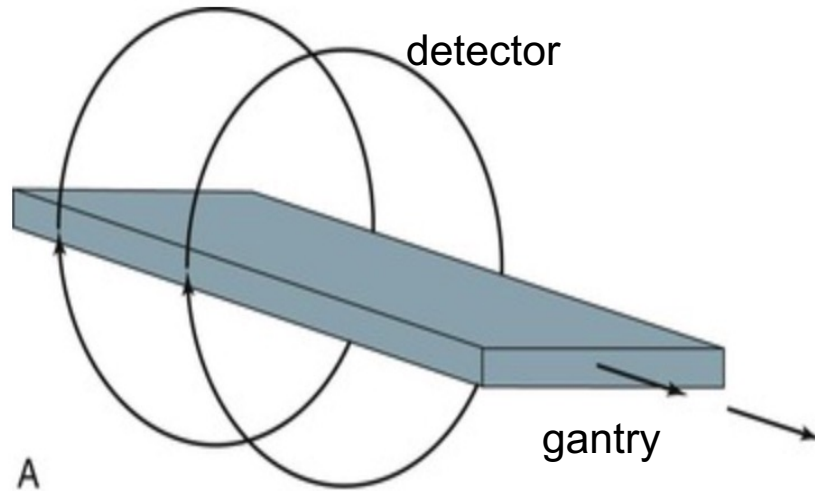


Image: J. Fessler. Image reconstruction: Algorithms and analysis. [5]

- β - angle of the source point counter-clockwise from the y axis
- (x_{β}, y_{β}) – rotated coordinates.
- Extra height parameter t in the detector.
- Other parameters are similar to fan-beam geometry described previously.
- Here, we consider only circular X-ray source trajectory (axial scan)
- Reconstruction algorithm used: **Feldkamp conebeam** algorithm or **FDK** approach

Short digression on Axial scan



- X-ray tube and detector are stationary
- Patient moved through the gantry for cross sectional image to be taken at that specific location.
- Multiple slices are stacked to create the image.

Image: <https://clinicalgate.com/computed-tomography-3/>

Equidistant case (flat detector)

- Forward projection: $p(s, t; \beta) = \int_{L(s, t; \beta)} f(x, y, z) dl$ (24)
- FDK algorithm:

- Step 1: Compute weighted projections using the projection weighting

$$\bar{p}(s, t; \beta) = w_1(s, t)p(s, t; \beta), \quad w_1(s, t) = \frac{D_{so}}{\sqrt{D_{sd}^2 + s^2 + t^2}} \quad (25)$$

- Step 2: Filter those projections along each row of the detector as if it were part of a 2D fan-beam acquisition using the ordinary ramp filter $h^*(s)$ from equation (20)

$$\bar{p}(s, t; \beta) = \bar{p}(s, t; \beta) * h_*(s) \quad (26)$$

$$h[n] = \begin{cases} 1, & n = 0 \\ 0, & n \text{ even} \\ \frac{-1}{(\pi n/2)^2}, & n \text{ odd} \end{cases}$$

- Step 3: Perform weighted cone-beam backprojection of those filtered projections

$$\hat{f}(x, y, z) = \frac{1}{2} \int_0^{2\pi} w_2(x, y, \beta) \bar{p}(s_\beta(x, y), t_\beta(x, y, z); \beta) d\beta \quad (27)$$

Reminder of
equation 20 !

$$w_2(x, y, \beta) = \frac{D_{sd}^2}{(D_{so} - y_\beta)^2} \quad s_\beta(x, y) = \frac{D_{sd}}{D_{so} - y_\beta} x_\beta \quad t_\beta(x, y, z) = \frac{D_{sd}}{D_{so} - y_\beta} z \quad (28)$$

Equiangular case (curved detector)

- Procedure is similar to the FDK algorithm
- Differences:

- Replace the 1D weighting equation (25) by: $w_1(s, t) = \frac{D_{s0}}{\sqrt{D_{sd}^2 + t^2}} \cos\left(\frac{s}{D_{sd}}\right)$ (29)

- Replace the filter in equation (26) with the modified ramp filter in equation (16)

$$h[n] = \begin{cases} \frac{1}{4\Delta_s^2}, & n = 0 \\ 0, & n \text{ even} \\ \frac{-1}{[\pi D_{sd} \sin(n\Delta_s/D_{sd})]^2}, & n \text{ odd} \end{cases} \quad (16) \quad \text{Reminder!}$$

- Replace weighting ratio w_2 in (28) with (17), s_β with (9) and t_β unchanged.

$$\frac{1}{W_2^2 L_\beta^2(x, y)} = \frac{D_{sd}^2}{L_\beta^2(x, y)} = \frac{D_{sd}^2}{(D_{s0} - y_\beta)^2 + (x_\beta - r_{off})^2} \quad (17)$$

$$s_\beta(x, y) = \begin{cases} D_{sd} \gamma_\beta(x, y), & \text{if } D_{fs} = 0 \text{ (equiangular)} \\ D_{sd} \tan \gamma_\beta(x, y), & \text{if } D_{fs} = \infty \text{ (equidistant)} \end{cases} \quad (9)$$

Topics

Introduction

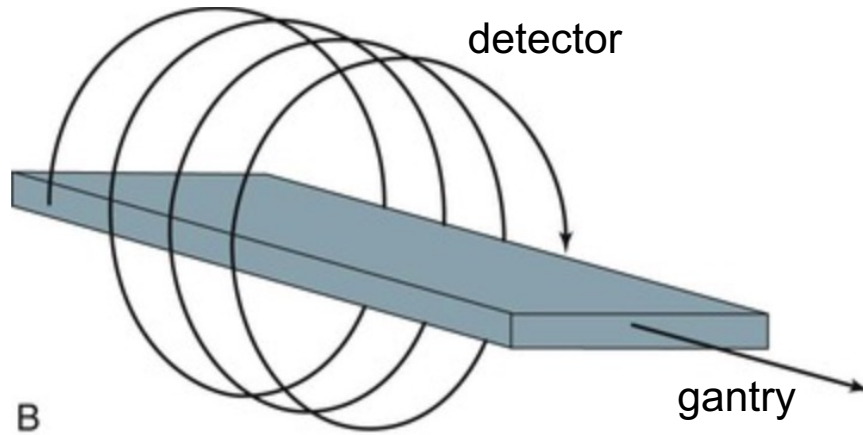
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Outlook on advanced methods

Conclusion

Helical (Spiral) scan



- Continuous rotation of the X-ray tube (emitter) and detector around the patient.
- Continuous data acquisition.
- More efficient than axial scanning, faster acquisition.
- More commonly in use today.
- Importantly, FBP type reconstruction exists.

Image: <https://clinicalgate.com/computed-tomography-3/>

Cone-parallel rebinning

- Simplified computation and reduced noise for both axial and helical scans.
- converts the fans for each detector row into cone-parallel rays.

$$p_{\text{CP}}(r, \varphi; t) \triangleq p(s, t; \beta) \Big|_{s=s(r), \beta=\beta(r, \phi)} = p\left(\gamma^{-1}\left(\arcsin\left(\frac{r}{D_{s0}}\right)\right), t; \phi - \arcsin\left(\frac{r}{D_{s0}}\right)\right)$$

where,

$$s(\gamma) = \gamma^{-1}(s) = \begin{cases} D_{sd}\gamma, & \text{if } D_{fs} = 0 \text{ (equiangular)} \\ D_{fd}[\gamma - \arcsin(\frac{D_{fs}}{D_{fd}} \sin \gamma)], & \text{if } 0 \leq D_{fs} \leq \infty \\ D_{sd} \tan \gamma, & \text{if } D_{fs} = \infty \text{ (equidistant)} \end{cases} \quad (2)$$

Topics

Introduction

2D fan beam tomography

3D cone-beam reconstruction

Outlook on advanced methods

Conclusion

Comparison

Geometries	Parallel-beam	Fan-beam	Cone-beam
Dimension	2D		3D
projection	$p(r, \phi)$	$p(s, \beta)$	$p(s, t, \beta)$
Reconstruction algorithm	FBP , BPF, CBP	“weighted” FBP, fan parallel-rebinning, BPF	FDK (axial)
Generation	1 st	3 rd	3 rd
Acquisition time	Slow	fast	faster

References

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The End
(and Thank you!!)

