Kinematics and Dynamics of an In-Parallel-Actuated Soft Robot Manipulator: Application to Cranial Cancer Radiosurgery

Olalekan Ogunmolu

Abstract—A completely soft multi-degree of freedom parallel robot alternative in 6-DOF real-time patient motion correction is here put forward to counterbalance the heretofore preoccupation with rigid in-parallel robot mechanisms in frameless and maskless radiosurgery. We study the kinematics using ideas from algebra and Group theory, as well as the contact dynamics between the soft actuators and the patient's head. We then analyze the forces that govern the interaction between the soft robots and the patient's head and neck region using differential geometry. Relating the solutions to the boundary value problem of the Cauchy stress for the soft robots to the contact force wrenches at the head and neck region, we synthesize the manipulation map and construct the associated Jacobian for their direct positioning analysis. Within the (isochoric and shear deformation) properties forthwith presented, the mechanism is intended to provide a minimally-invasive motion-correction in lieu of the rigid frames and masks in clinics today. Our goal is to edge open the door a little further towards in-parallel soft actuation mechanisms that do not attenuate the radiation beam, are non-invasive, and are comfortable for the patient whilst preserving radiation dose efficacy and treatment efficiency; others may then improve upon this with ablative versions of the presented mechanism, or with more efficient analytic or numerical apparatus for the Jacobian and dynamics. This is a work in progress and suggestions are welcome.

I. INTRODUCTION

This work is principally a continuation of the model verified in [3]. Here, we present the systematic analysis of the inparallel-actuated mechanism. The possible major application is towards a real-time closed-loop automatic motion deviationcorrection, particularly during beam-on time, in robotic radiosurgery; this is a desperately needed technology that has the potential benefits of hastening the current treatment time in clinics, minimizing patient discomfort post-treatment (as opposed to rigid frames and masks used in frame and maskbased RT), and drastically improving dose efficacy so that the patient's treatment can be effectively fractionated [4]. It could also find applications in the animation industry where animated plushes are required to be accurately actuated so as to yield a desired configuration for users [5], [6]. The real-time control of hyperelastic materials is another possible application [7], [8].

We call the individual soft robots inflatable air bladders (IABs) owing to their hollow internal chambers that admit or eject air based on an applied internal pressurization. We

Perelman School of Medicine, The University of Pennsylvania, Philadelphia, PA 19104, USA. Olalekan.Ogunmolu@pennmedicine.upenn.edu

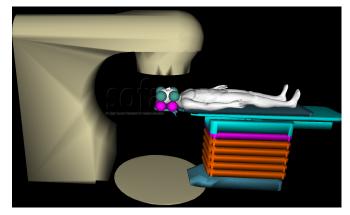
make the fundamental assumption that the IAB's deformation follows the isochoric deformation principle, with reasonable local volume preservation during deformation constraints baked into the physical IAB material properties. We derive the manipulator map, kinematics, Jacobian and end-effector velocities. Soft robots are notoriously difficult to control, given their continuum-based mechanical properties, and the interdependency of the parameters that characterize their deformation. It is not surprising that different schemes for controlling soft continuum robots have appeared in literature with mixed successes [9]–[15]. For an extensive literature review of the control of continuum soft robots, we refer readers to [16].

The soft robot mechanism consists of IABs connected with extensible couplings; these couplings are chosen to exploit the soft structures' design for impedance control of the H&N region of the patient. We analyze the manipulation map, the Jacobian of the IAB chains, as well as the contact equations between the IAB mechanism system and patient's cranial region. This paper is a sequel to our previous works [4], [10], [17]–[19]; additionally, we expand upon the kinematics and dynamics of the multi-DOF soft actuation system for H&N motion compensation in RT. Our design goals include a system that (1) provides patient comfort whilst manipulating human body parts necessary for trajectory following during RT, (2) assures dose efficacy while not attenuating the ionizing radiation dose treatment due to undesirable material properties (3) capable of emerging complex morphological computational behavior with deformable soft robots - simplifying complex patient motion planning and control during robotic RT treatment.

The rest of this paper is organized as follows:we analyze the contact kinematics in § IV, describing the contact model, and how we solve the boundary value problem for the IABs' deformation. In § V, we derive the mechanism's end-effector velocities and forces, and then derive the Newton-Euler Lagrangrian relationship in § III. We present manipulation examples in the SOFA framework in ?? and conclude the paper in § VII. Proofs and derivations are provided in appendices A, B, and C.

II. IAB DEFORMATION: A MACROSCOPIC CHARACTERIZATION

For a background material on this section, readers are encouraged to read [4, §2-§3] and [20]. At a material point X of the IAB surface in a configuration \mathcal{B}_{\circ} , it can be verified



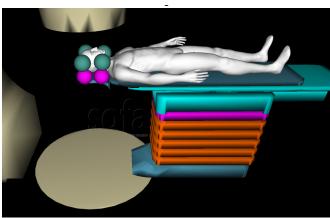


Fig. 1. System setup in the SOFA Framework Architecture. **Top**: Gantry, Turntable, Patient and IAB Chains around the patient's H&N Region. **Bottom**: Close-up view of compensating IABs around patient's H&N region with the patient lying in a supine position on the treatment couch. [Image best visualized in colored ink].

that the tensor $\mathbf{C} - \mathbf{I}$ represents a change in length of an arbitrary line element of the material, where \mathbf{C} is the right Cauchy-Green Tensor as defined in [3]. For the material to be unstrained, we must have the Lagrangean strain tensor as zero i.e.

$$\mathbf{E} = \frac{1}{2} \left(\mathbf{C} - \mathbf{I} \right) = 0.$$

A particle **X**'s displacement from the reference to the current configurations must be such that the point difference $d = \mathbf{x} - \mathbf{X}$ is $d(\mathbf{X}) = \chi(\mathbf{X}) - \mathbf{X}$, where $\chi(\mathbf{X})$ follows our notation in [3]. We can therefore characterize the point differences by the two-point displacement gradient,

$$\mathbf{D} = \text{Grad } d(\mathbf{X}) = \mathbf{F} - \mathbf{I}. \tag{1}$$

If we define unit vectors \mathbf{m} and \mathbf{M} tangent to fibers \mathbf{dx} and \mathbf{dX} in the current and reference configurations respectively, it follows from the invariant of deformation that

$$\mathbf{m}|\mathbf{dx}| = \mathbf{FM}|\mathbf{dX}| \implies |\mathbf{dx}|^2 = \mathbf{M} \cdot (\mathbf{CM})|\mathbf{dX}|^2.$$
 (2)

Whence, the *stretch* between line elements dx and dX is

$$\lambda(\mathbf{M}) = \frac{|\mathbf{dx}|}{|\mathbf{dX}|} = |\mathbf{FM}| = (\mathbf{M} \cdot (\mathbf{CM}))^{\frac{1}{2}}.$$
 (3)

Lastly, we define two line elements dX and dX' with unit tangent vectors M and M' at points X and X' in the reference

configuration; these fibers correspond to dx and dx' with unit vectors \mathbf{m} and \mathbf{m}' at points \mathbf{x} and \mathbf{x}' in the current configuration. Let β denote the angle between the directions \mathbf{M} and \mathbf{M}' and let α be the angle between directions \mathbf{m} and \mathbf{m}' ; then

$$\mathbf{dx} = \mathbf{FdX}, \quad \mathbf{dx'} = \mathbf{FdX'}, \quad \beta = \cos^{-1}(\mathbf{M} \cdot \mathbf{M'}), \quad (4a)$$

and $\alpha = \cos^{-1}(\mathbf{m} \cdot \mathbf{m'}) = \cos^{-1}(\mathbf{M} \cdot (\mathbf{CM'})/\lambda(\mathbf{M}) \cdot \lambda(\mathbf{M'})).$
(4b)

In the plane of shear of M and M', the *angle of shear* between the material line elements is the reduction in angles

$$\phi = \beta - \alpha. \tag{5}$$

Examining (1), and (3), we notice that they are both characterized by the stretch $\lambda=r/R$ and the radius in the current configuration (c.f. [3]). Therefore, we take the kinematic quantities that characterize the IAB deformation as

$$\mathbf{r} = \begin{bmatrix} \lambda \\ r \\ \phi \end{bmatrix} = \begin{bmatrix} r/R \\ (R^3 + r_i^3 - R_i^3)^{1/3} \\ \beta - \alpha \end{bmatrix}$$
(6)

i.e. \mathbf{r} is a function of material stretch, the angle of shear between material line elements, and the shell radius, r as derived in [3]. Therefore, we have

Generalized Coordinates $\mathbf{r} = \begin{bmatrix} \lambda \\ r \\ \phi \end{bmatrix} = \begin{bmatrix} r/R \\ (R_o^3 + r_i^3 - R_i^3)^{1/3} \\ \beta - \alpha \end{bmatrix} \tag{7}$

as the generalized coordinates of an IAB within the mechanism.

III. SYSTEM'S NEWTON-EULER EQUATIONS

From Truesdell's determinism for the stress principle [21], the Cauchy stress σ at any point in a material at time t for any motion up to time t determines the stress response of the material for any arbitrary motion history up to and including time t. We will derive the dynamics of the IAB system in the strain field of the deformation. The potential and kinetic energy of the system are considered to be derived from the constitutive strain field relations that characterize the deformation. We now use Lagrangian deformation analysis to derive the dynamic equations of the continuum multi-IAB system.

For a soft continuum body, there is an enormous amount of particle orientations during deformation; the number of particle states that is physically measurable with sensors instantaneously in a given configuration is overwhelming. However, we can leverage the constitutive law which describes the macroscopic IAB material behavior with respect to a reference frame, S, at a time, t by completely characterizing it by ten dependent variables viz., three components of the position vector, six component stress tensor variables (the shear and normal stress components), and

A. Lagrangian and Euler-Lagrange Equations

Following § II, we are only interested in the final position and orientation of the IAB as a whole rather than the system of particles that characterize a deformation at every time t. When the head exerts a reactive wrench on an IAB, it is natural to expect a dent. The shear angle in (7) should capture the amount of angular deformation. For a kinetic energy T and a potential energy V, the Lagrangian, L, of the system in generalized coordinates is the difference between the kinetic and potential energy, i.e.

$$L(\mathbf{r}, \dot{\mathbf{r}}) = T(\mathbf{r}, \dot{\mathbf{r}}) - V(\mathbf{r}). \tag{8}$$

The equations of motion for a pneumatic IAB system is of the form

$$\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}_i} - \frac{\partial L}{\partial \mathbf{r}_i} = \boldsymbol{\tau}_i, \quad i = 1, \dots, m$$
(9)

where τ_i is the torque acting on the i^{th} generalized coordinate. Written in matrix form equation, we can write the Euler-Lagrange equation of (9) as

$$\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \mathbf{r}} = \boldsymbol{\tau}.$$
 (10)

It now remains to derive the kinetic and potential energies for the IAB material. Let the velocity of an IAB material particle \mathbf{x} in the current configuration at time t be $\mathbf{v}(\mathbf{r},t)$, then the Eulerian velocity gradient tensor can be defined as

$$\Gamma = \text{grad } \mathbf{v}(\mathbf{r}, t). \tag{11}$$

Cauchy's first law of motion (24a) will allow us to derive the balance of mechanical energy of the system. Multiplying(24a) throughout by $\mathbf{v}(\mathbf{r},t)$, and abusing notation by dropping the arguments of $\mathbf{v}(\mathbf{r},t)$, we find that

$$\operatorname{div} (\boldsymbol{\sigma}^{T} \cdot \mathbf{v}) + \rho \mathbf{b} \cdot \mathbf{v} = \rho \mathbf{v} \cdot \dot{\mathbf{v}}$$

$$\implies \operatorname{div} (\boldsymbol{\sigma}^{T} \mathbf{v}) - \operatorname{tr}(\boldsymbol{\sigma} \boldsymbol{\Gamma}) + \rho \mathbf{b} \cdot \mathbf{v} = \rho \mathbf{v} \cdot \dot{\mathbf{v}}. \tag{12}$$

Following mass conservation, we integrate over volume \mathcal{B} and employ the divergence theorem, so that the above relation yields the *balance of mechanical energy*:

$$\int_{\mathcal{B}} \rho \mathbf{b} \cdot \mathbf{v} \, dv + \int_{\partial \mathcal{B}} f_{\rho} \cdot \mathbf{v} \, da = \frac{d}{dt} \int_{\mathcal{B}} \frac{1}{2} \rho \mathbf{v} \cdot \mathbf{v} \, dv + \int_{\mathcal{B}} \mathbf{tr}(\boldsymbol{\sigma} \, \boldsymbol{\Gamma}) \, dv$$
(13)

where f_{ρ} is the IAB body force density, and the left hand side of the foregoing is the so-called *rate of working of the applied forces*. The symmetry of the stress tensor σ implies that $\mathbf{tr}(\sigma \Gamma) = \mathbf{tr}(\sigma \Sigma)$ where Σ is given in terms of the Eulerian-strain rate tensor, Γ *i.e.*

$$\Sigma = \frac{1}{2}(\mathbf{\Gamma} + \mathbf{\Gamma}^T) \tag{14}$$

so that the kinetic energy density and stress power are given by,

$$T(\mathbf{r}, \dot{\mathbf{r}}) = \frac{1}{2} \rho \mathbf{v} \cdot \mathbf{v}, \quad V(\mathbf{r}) = \mathbf{tr}(\boldsymbol{\sigma} \, \boldsymbol{\Sigma}). \tag{15}$$

B. Case I: Dynamics for Cauchy-Elastic IAB Materials

The stress-strain relation for the IAB we have presented are only related through the deformation tensor, implying that the material is Cauchy elastic. For Cauchy elastic materials, the stress power term is not conserved during deformation making integration over the material body $\mathcal B$ physically unrealistic [20]. For such materials, we may set the stored strain energy V to an arbitrary constant (e.g. an identity or V(I)=0). We can derive the overall torque dynamics of an IAB system as (see proof in Appendix A)

$$\frac{2\|\mathbf{r}\|^{2}}{\rho}\boldsymbol{\tau} = \underbrace{\begin{bmatrix} 1/R^{2} & 0 & 0 \\ 0 & 9r_{i}^{4} & 0 \\ 0 & 0 & \|\mathbf{r}\|^{2} \end{bmatrix}}_{M_{iab}} \begin{bmatrix} \ddot{r} \\ \ddot{r}_{i} \\ \ddot{\alpha} \end{bmatrix} + \underbrace{\begin{bmatrix} -2/R & 0 & 0 \\ 0 & 36r_{i}^{3} & 0 \\ 0 & 0 & 0 \end{bmatrix}}_{G} \begin{bmatrix} \dot{r} \\ \dot{r}_{i} \\ \dot{\alpha} \end{bmatrix}. \tag{16}$$

Rewriting equation (16) in terms of the torque for each soft robot, we have the dynamics for IAB j as

$$M_{iab_j}(R, r_i{}^j, \mathbf{r})\ddot{\mathbf{r}}_j + C_{iab_j}(R, r_i^j)\dot{\mathbf{r}}_j = \frac{2\|\mathbf{r}\|^2}{\rho}\boldsymbol{\tau}_j$$
(17)

where M_{iab_j} and C_{iab_j} contain the respective inertia and Coriolis forces for actuator j, and r_i^j, τ_j are respectively the internal radius and actuator torque of the j'th IAB. Since the IAB material is incompressible, the mass density is uniform throughout the body of the material. In general, we write equation (17) as

$$M_{iab}(\tilde{\mathbf{r}})\ddot{\tilde{\mathbf{r}}} + C_{iab}(\tilde{\mathbf{r}},\dot{\tilde{\mathbf{r}}})\dot{\mathbf{r}} = \frac{2\|\tilde{\mathbf{r}}\|^2}{\rho}\tilde{\boldsymbol{\tau}}$$
(18)

where $\tilde{\mathbf{r}} \in \mathbb{R}^{n_1} \times \mathbb{R}^{n_2} \times \cdots \mathbb{R}^{n_8}$ gives the generalized coordinates for all the IABs and $\tilde{\tau}$ are the vectorized torques of the individual robots.

C. Case II: Dynamics for Green Elastic IAB Materials

For the case where the IAB material body is *Green elastic* or *hyperelastic*¹, the eulerian form of the stress power expression is

$$V(\mathbf{r}) = \mathbf{tr}(\boldsymbol{\sigma}\,\boldsymbol{\Sigma}). \tag{19}$$

We are mostly interested in the mechanical energy in the current configuration, however, it is worthwhile to note that the equivalent relation in the Lagrangean form is

$$\int_{\mathcal{B}_{\circ}} \rho_{\circ} \mathbf{b}_{\circ} \dot{\boldsymbol{\chi}} \, dV + \int_{\partial \mathcal{B}_{\circ}} (\mathbf{S}^{T} \mathbf{N}) \dot{\boldsymbol{\chi}} \, dA =
\frac{d}{dt} \int_{\mathcal{B}_{\circ}} \frac{1}{2} \rho_{\circ} \, \dot{\boldsymbol{\chi}} \cdot \dot{\boldsymbol{\chi}} \, dV + \int_{\mathcal{B}_{\circ}} \mathbf{tr} (\mathbf{S} \dot{\mathbf{F}}) \, dV, \qquad (20)$$

where S is the piola-kirchoff stress tensor. It follows that,

$$V(\mathbf{r}) = \mathbf{tr}(\mathbf{S}\dot{\mathbf{F}}) \tag{21}$$

for a Green elastic material.

¹An hyperelastic material is one where the strain-energy function exists.

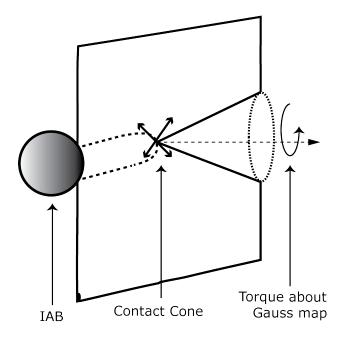


Fig. 2. Illustration of the IAB Soft Contact Type

IV. ANALYSIS OF CONTACT KINEMATICS

The manipulators and head are considered as linear elastic object materials with the interaction at the head and an IAB contact considered as a classical case of two elastic bodies in contact. We model the contact type between the head and an IAB similar to the soft finger contact primitive of [23]. Here, our soft contact is the convex sum of *point contacts* with friction over the small area of contact. IAB forces and torques are modeled within a "cone of forces" about the direction of the surface normal from a patient's head (see Figure 2). The trajectory of the head under the influence of motion of an IAB is influenced by the position vector \mathbf{r} described in [3]. When the IAB deforms, body forces over its current configuration and contact (*traction*) forces over its boundary $\partial \mathcal{B}$ impact motion on the head. Constrained by the frictional coefficient, we define the soft contact force inside the friction cone as

$$\tilde{F}_{c_i} = \begin{bmatrix} \mathbf{I} & 0 \\ 0 & n_{c_i} \end{bmatrix} \begin{bmatrix} f_{c_i} \\ \tau_{c_i} \end{bmatrix}, \tag{22}$$

where $f_{c_i} \in \mathbb{R}^3$ denotes the amount of force exerted by the IAB along the direction of contact, $\tau_{c_i} \in \mathbb{R}$ is the moment of the contact force, and n_{c_i} is the normal or Gauss map² for a manifold $S \subset \mathbb{R}^3$ of a head surface. For contact models with friction, we require that all contact forces lie within the friction cone, determined by the frictional coefficient. The set of forces within or on the boundary of the friction cone is

$$FC = \{ f_c \in \mathbb{R}^n : ||f_{c_{ij}}^t|| \le \mu_{ij} ||f_{c_i}^n||,$$

$$i = 1, \dots, k, j = 1, \dots, m_i \}$$
(23)

where $f_{c_{ij}}^t$ is the tangent component of the j^{th} element of the contact force, $f_{c_i}^n$ is i^{th} contact's normal force, and μ_{ij} is $f_{c_{ij}}$'s coefficient of friction.

A. Boundary Value Problem for IAB Deformation

In general, we expect the isochoric deformation principle to hold for the side IAB chains and that our analysis in [3] holds for these actuators. For these actuators, the position vector on the IAB material body is given by (7) with ϕ set to zero. We now solve the boundary-value problem for the IAB deformation when the head rests on the base IABs. Again, we assume a spherically-symmetric deformation constraint imposed on the IAB when the head rolls or slips. For an IAB material, when the SoRos are in contact with the head, the applied forces on the current configuration of the IAB body $\mathcal B$ are

- the body forces, b
- the contact forces, f_c , at the IAB boundary, $\partial \mathcal{B}$, and
- the gravitational force of the head mass acting along the direction of contact, f_q .

We make the explicit assumption that the head maintains contact with the IAB throughout deformation. This is a reasonable assumption given the tight kinematic arrangement around the cranial region as sen in Figure 1. Suppose that for the i^{th} IAB in the chain, r_{c_i} represents the direction vector perpendicular from the point of contact to the center of the head cone of forces, it follows that the three equations that govern the motion of the IAB continuum are given as

$$\dot{\rho} + \rho \operatorname{div} \mathbf{v} = 0 \tag{24a}$$

$$\boldsymbol{\sigma}^T = \boldsymbol{\sigma} \tag{24b}$$

$$\operatorname{div} \boldsymbol{\sigma}^T + \rho \boldsymbol{b} = \rho \dot{\mathbf{v}}, \tag{24c}$$

being respectively the conservation of mass (24a), the symmetry of the stress tensor (24b), and the balance of linear momentum respectively, (see [20, pp. 150], for the derivation). In general, we expect that the mass of the body will be conserved given the incompressibility assumption of the IAB material, thus guaranteeing that (24a) is fulfilled. We have from (24c) and the symmetric properties of the stress tensor that

$$\frac{1}{r^2} \frac{\partial}{\partial r} (r^2 \sigma_{rr}) + \frac{1}{r \sin \phi} \frac{\partial}{\partial \phi} (\sin \phi \sigma_{r\phi}) + \frac{1}{r \sin \phi} \frac{\partial}{\partial \theta} (\sigma_{r\theta})
- \frac{1}{r} (\sigma_{\theta\theta} + \sigma_{\phi\phi}) + \rho b_{\lambda} = \rho \ddot{\lambda}$$
(25a)
$$\frac{1}{r^3} \frac{\partial}{\partial r} (r^3 \sigma_{r\phi}) + \frac{1}{r \sin \phi} \frac{\partial}{\partial \phi} (\sin \phi \sigma_{\phi\phi}) + \frac{1}{r \sin \phi} \frac{\partial}{\partial \theta} (\sigma_{\theta\phi})
- \frac{\cot \phi}{r} (\sigma_{\theta\theta}) + \rho b_{\phi} = \rho \ddot{r}$$
(25b)
$$\frac{1}{r^3} \frac{\partial}{\partial r} (r^3 \sigma_{\theta r}) + \frac{1}{r \sin^2 \phi} \frac{\partial}{\partial \phi} (\sin^2 \phi \sigma_{\theta\phi})
+ \frac{1}{r \sin \phi} \frac{\partial}{\partial \theta} (\sigma_{\theta\theta}) + \rho b_{\theta} = \rho \ddot{\phi}$$
(25c)

where the body forces b_r, b_ϕ, b_θ are components of the gravitational force of the head acting on the IAB body B. It follows that the forces on the head (see derivation in Appendix

 $^{^2}$ A normal map for a manifold S is a continuous map $g: S \to S^2 \subset \mathbb{R}^3$ such that for every $s \in S, g(s)$ is orthogonal to S at s [24].

A) are in part the internal pressurization, and component stresses $\{P_i, \sigma_{\phi\phi}(\epsilon), \sigma_{\theta\theta}(\zeta)\}$ as given in (26)

$$\begin{split} P &= \int_{r_i}^{r_o} \left[\frac{1}{r} \left(-2p + 2C_1 \frac{r^2}{R^2} - 2C_2 \frac{R^8}{r^8} \right) - \rho b_r \right. \\ &+ \rho \cos \theta \left(2\dot{r}\dot{\phi}\cos\theta + r\cos\theta \ddot{\phi} - 2r\dot{\theta}\dot{\phi}\sin\theta \right) - \rho \sin\phi \\ &\left. \left(\cos\theta (-\ddot{r} + r\dot{\theta}^2 + r\dot{\phi}^2) + \sin\theta (2\dot{r}\dot{\theta} + r\ddot{\theta}) \right) \right] dr \end{split} \tag{26a}$$

$$\sigma_{\phi\phi}(\epsilon) = -\int_{\epsilon}^{\pi} \left[r\rho \left[\cos\phi \left(2r\dot{\theta}\dot{\phi}\cos\theta + (2\dot{r}\dot{\phi} + r\ddot{\phi})\sin\theta \right) \right. \right. \\ \left. + \sin\theta \left(2\dot{r}\dot{\theta}\cos\theta + r\ddot{\theta}\cos\theta + (\ddot{r} - r\dot{\theta}^2 - r\dot{\phi}^2) \right) \sin\phi \right] \\ \left. - \rho rb_{\theta} \right] d\phi, \ 0 \le \epsilon \le \pi$$

$$\left. (26b)$$

$$\sigma_{\theta\theta}(\zeta) = -\int_{\zeta}^{2\pi} \left[-r\rho b_{\theta}\sin\phi + r\rho\sin\phi\cos\phi \left(\ddot{r} - r\dot{\phi}^2 \right) \right. \\ \left. - r\rho\sin^2\phi \left(2\dot{r}\dot{\phi} + r\ddot{\phi} \right) \right] d\theta, \ 0 \le \zeta \le 2\pi,$$

$$\left. (26c)$$

where $0 \le \epsilon \le \pi$, and $0 \le \zeta \le 2\pi$.

B. Contact Forces, IAB Stress Components, and Head Gravitational Force

Here, we relate the microscopic contact stress of the previous section with the macroscopic descriptions of the contact friction to enable us treat different material combinations for the manipulator and head. We assume that the stress vector σ at a point on the IAB surface is uniform and continuous throughout the IAB boundary so that it linearly depends on the normal map (this follows from Cauchy's theorem; readers may see the proof in [20, §3.3.1]). Recall that the correspondence between material line, $\{dx, dX\}$, elements in the reference and current configuration is

$$\mathbf{dx} = \mathbf{F} \, \mathbf{dX} \implies \mathbf{F}^{-T} \mathbf{dx} = \mathbf{dX}.$$
 (27)

where \mathbf{F} is the deformation gradient. Let $\mathbf{H} = \mathbf{F}^{-T}$ and \mathbf{dA} represent an infinitesimal vector element on the material surface at a neighborhood of point \mathbf{X} in \mathcal{B} such that $\mathbf{dA} = \mathbf{N}\mathbf{dA}$, where \mathbf{N} is the unit outward normal to the IAB boundary $\partial \mathcal{B}_{\circ}$ in the reference configuration. The corresponding deformed surface of the IAB with normal \mathbf{n} from a surface, da, of the IAB in the current configuration is $\mathbf{da} = \mathbf{n}$ da. Using *Nanson's formula*, we have the following relation between surfaces in the reference and current configuration

$$d\mathbf{a} = J \mathbf{H} d\mathbf{A} \implies \mathbf{n} d\mathbf{a} = J \mathbf{H} \mathbf{N} d\mathbf{A}.$$
 (28)

where $J = \det \mathbf{F}$. Multiplying throughout equation (28) by the derived constitutive relation between the stress-strain relationship of [3], the resultant contact force on the boundary $\partial \mathcal{B}$ in the current configuration may be written as (owing to the volume preservation on the boundary of the IAB material)

$$\int_{\partial \mathcal{B}} \boldsymbol{\sigma} \, \mathbf{n} \, \mathrm{da} = \int_{\partial \mathcal{B}_{0}} J \, \boldsymbol{\sigma} \, \mathbf{H} \, \mathbf{N} \, \, \mathrm{dA}. \tag{29}$$

We may define the Piola-Kirchoff stress tensor field as

$$\mathbf{S} = J \mathbf{H}^T \boldsymbol{\sigma} \tag{30}$$

so that the force on an element surface da of the IAB in a configuration $\mathcal B$ is

$$\sigma da = S^T dA$$
.

Thus, the contact force f_{c_i} on the boundary $\partial \mathcal{B}$ of the i^{th} IAB in a configuration \mathcal{B} (as in (22)) is

$$f_{c_i} = \mathbf{S}_i^T \mathbf{d} \mathbf{A}_i = J_i \boldsymbol{\sigma}_i \mathbf{H}_i \mathbf{d} \mathbf{A}_i = J_i \boldsymbol{\sigma}_i \mathbf{F}_i^{-1} \mathbf{d} \mathbf{A}_i$$
 (31)

where (31) follows from the symmetric property of \mathbf{F}_i and σ_i . For the i^{th} IAB, at the region of contact, we have the contact force as

$$f_{c_i} = J_i \left(\frac{R_i^2}{r_i^2} P_i + \frac{R_i}{r_i} \sigma_{\phi\phi_i}(\epsilon) + \frac{R_i}{r_i} \sigma_{\theta\theta_i}(\zeta) \right) \mathbf{dA}_i \qquad (32)$$

where $\sigma_{jj_i}(v)$ are the definite integrals of (26). Owing to the isochoric deformation assumption, we have from (32) that

$$f_{c_i} = \left(\frac{R_i^2}{r_i^2} P_i + \frac{R_i}{r_i} \sigma_{\phi\phi_i}(\epsilon) + \frac{R_i}{r_i} \sigma_{\theta\theta_i}(\zeta)\right) n_{c_i} dA_i.$$
 (33)

where we have set the outward normal map N to n_{c_i} of (22). The torque is the moment of the contact force on the i^{th} IAB, and it is given by

$$\tau_{c_i} = f_{c_i} \times r_{c_i} \tag{34}$$

where $r_{c_i} \in \mathbb{R}^3$ is the unit vector between the head reference point and the contact. The soft contact force of (22) can be re-stated in terms of the derived stress tensor, the deformation gradient (see [3]) and the Piola-Kirchoff stress field of (30) *i.e.*

Friction Cones' Contact Force

$$\tilde{F}_{c_i} = \begin{bmatrix} \mathbf{I} & 0 \\ 0 & n_{c_i} \end{bmatrix} \begin{bmatrix} f_{c_i} \\ f_{c_i} \times r_{c_i} \end{bmatrix}. \tag{35}$$

where f_{c_i} and τ_{c_i} are as given in equations (33) and (34).

C. Contact Coordinates and Head Velocity

The head will make contact with the IAB at multiple points on its surface, so we describe the kinematics of these contact points using an atlas³ of contact coordinate charts. In this sentiment, let C_{r_1} and C_{r_h} respectively represent a fixed reference frame with respect to the IAB and head, H (see Figure 3). Furthermore, let $S_1 \subset \mathbb{R}^3$ and $S_h \subset \mathbb{R}^3$ denote the respective orientable manifold⁴ embeddings of the IAB and head surfaces with respect to frames C_{r_1} and C_{r_h} . We shall let S_1 and S_r belong to the atlases $\{S_{1_i}\}_{i=1}^{n_1}, \{S_{h_i}\}_{i=1}^{n_r}$ respectively. Suppose (f_1, U_1) and (f_r, U_r) are coordinate systems for the IAB and the head respectively, where f_i is an invertible map, $f_i(u_i, v_i): U \to S_i \subset \mathbb{R}^3$

$$f_i(u_i, v_i) : \{U \to S_i \subset \mathbb{R}^3 | i = 1, h\},$$

 3 An atlas \tilde{S} is a set of surfaces where each surface $S \in \tilde{S}$ has an invertible map $f(\boldsymbol{u})$ from an open subset U of \mathbb{R}^2 to a surface $S \subset \mathbb{R}^3$ such that the partial derivatives $\frac{\partial f}{\partial u}(\boldsymbol{u}), \, \frac{\partial f}{\partial v}(\boldsymbol{v})$ are linearly independent for all $\boldsymbol{u} = (\boldsymbol{u}, \boldsymbol{v}) \in U$.

 4 An orientable manifold is a manifold S for which the Gauss map exists.

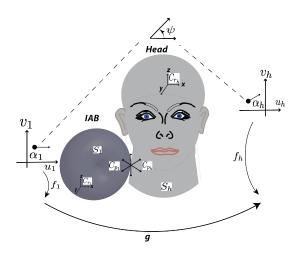


Fig. 3. Sliding and rolling contact illustration of a single IAB and the Head. [Image best visualized in colored ink].

from an open subset U of \mathbb{R}^2 to a coordinate patch $S_i \subset \mathbb{R}^3$ such that the partial derivatives $\frac{\partial f_i}{\partial u_i}$ and $\frac{\partial f_i}{\partial v_i}$ are linearly independent. Let $p_1(t) \in S_1$ and $p_h(t) \in S_h$ represent the positions of the contact points with respect to frames C_{r_1} and C_{r_h} respectively at time t. In general, the contact points $p_1(t)$ and $p_h(t)$ will not remain in the coordinate systems S_1 and S_h for all time. Thus, we choose an interval I where $p_1(t) \in S_{1_i}$ and $p_h(t) \in S_{h_j}$ for all $t \in I$ and some i and j. As seen in Figure 3, C_{p_1} and C_{p_h} denote the contact frames that coincide with the normalized Gauss frames at p_1 and p_h for all $t \in I$, and α_1 , α_h are local coordinate frames that describe the IAB motion with respect to the head such that

$$\alpha_1 = (u_1, v_1) \in U_1$$
, and $\alpha_h = (u_h, v_h) \in U_h$. (36)

Let the angle between the tangent planes of α_1 , and α_h be ψ . The transformation matrix $g \in \Omega \subset SE(3)$ encodes the relative orientation and position of the IAB with respect to the head where Ω is the set of all relative positions and orientations in the atlasses $\{S_{1_i}\}_{i=1}^{n_1}$, $\{S_{h_i}\}_{i=1}^{n_h}$ for which the IAB and head remain in contact. We let the *contact coordinates* be described by $\eta = (\alpha_1, \alpha_h, \psi)$. The head's motion is governed by traction forces arising from the friction tangential to the IAB surface and the pressure normal to the IAB surface. Thus, at the points of contact, if $R \in SO(3)$ is the rotatory component of g, η must satisfy

$$g \circ f_1(\alpha_1) = f_h(\alpha_h) \tag{37a}$$

$$R n_1(\alpha_1) = -n_h(\alpha_h) \tag{37b}$$

since the contact locations must coincide for the IAB and the head, and the tangent planes must coincide so that the outward normal maps $n_1:S_1\to S^2\subset\mathbb{R}^3$ and $n_h:S_h\to S^2\subset\mathbb{R}^3$ agree. Furthermore, the orientation of the tangent planes of α_1 and α_h is the unique angle $\psi\in[0,2\pi)$ between the x-axes of C_{p_1} and C_{p_h} such that

$$R\frac{\partial f_1}{\partial \alpha_1} M_1^{-1} R_{\psi} = \frac{\partial f_h}{\partial \alpha_h} M_h^{-1} \tag{38}$$

where M_i is a 2×2 square root of the Riemannian metric tensor [25] that normalizes the columns of $\frac{\partial f}{\partial \alpha}$, *i.e.*

$$M_{i} = \begin{bmatrix} \|\frac{\partial f_{i}}{\partial u_{i}}\| & 0\\ 0 & \|\frac{\partial f_{h}}{\partial v_{i}}\| \end{bmatrix}$$
(39)

and R_{ψ} is chosen such that a rotation of C_{p_1} about its z-axis through $-\psi$ radians aligns the x-axes of the local coordinate system α_1 to that of the head's local coordinate system α_h i.e.

$$R_{\psi} = \begin{bmatrix} \cos \psi & -\sin \psi \\ -\sin \psi & -\cos \psi \end{bmatrix} \tag{40}$$

with the special property that $R_{\psi} = R_{\psi}^T = R_{\psi}^{-1}$. We define the normalized Gauss frame at a point u on the surface U of the orthogonal coordinate system (f, U) as,

$$\begin{bmatrix} x_u & y_u & z_u \end{bmatrix} = \begin{bmatrix} \frac{\partial f}{\partial u} / \| \frac{\partial f}{\partial u} \| & \frac{\partial f}{\partial v} / \| \frac{\partial f}{\partial v} \| & n_u(f(u)) \end{bmatrix}$$
(41)

where x_u, y_u , and z_u are functions mapping $U \subset \mathbb{R}^2 \to \mathbb{R}^3$ and n_u is the continuous Gauss map $n_u : S \to S^2 \subset \mathbb{R}^3$. The motion of the contacts $\dot{\eta}$ as a function of components of the twist vector $\hat{\xi} = (v, w)^T$ is given in (42) as the respective first, second, and third equations of contact. Our derivation, which closely follows [26]'s multi-fingered kinematics' proof, may be found in Appendix B.

$$\dot{\alpha}_h = M_h^{-1} (\mathcal{K}_h + \tilde{\mathcal{K}}_1)^{-1} \left(\omega_t - \tilde{\mathcal{K}}_1 v_t \right) \tag{42a}$$

$$\dot{\alpha}_1 = M_1^{-1} R_{\psi} (\mathcal{K}_h + \tilde{\mathcal{K}}_1)^{-1} (\omega_t - \mathcal{K}_h v_t)$$
 (42b)

$$\dot{\psi} = \omega_n + T_h M_h \dot{\alpha}_h + T_1 M_1 \dot{\alpha}_1 \tag{42c}$$

where

$$T_{h} = y_{h}^{T} \frac{\partial x_{h}}{\partial \alpha_{h}} M_{h}^{-1}, \quad T_{1} = y_{1}^{T} \frac{\partial x_{1}}{\partial \alpha_{1}} M_{1}^{-1},$$

$$\mathcal{K}_{h} = \begin{bmatrix} x_{h}^{T}, & y_{h}^{T} \end{bmatrix}^{T} \frac{\partial n_{h}^{T}}{\partial \alpha_{h}} M_{h}^{-1}, \quad \omega_{n} = z_{h}^{T} \omega$$

$$\mathcal{K}_{1} = R_{\psi} \begin{bmatrix} x_{1}^{T}, & y_{1}^{T} \end{bmatrix}^{T} \frac{\partial n_{1}^{T}}{\partial \alpha_{1}} M_{1}^{-1} R_{\psi},$$

$$\omega_{t} = \begin{bmatrix} x_{h}^{T}, & y_{h}^{T} \end{bmatrix}^{T} \begin{bmatrix} n_{h} \times \omega \end{bmatrix}^{T},$$

$$v_{t} = \begin{bmatrix} x_{h}^{T}, & y_{h}^{T} \end{bmatrix}^{T} \begin{bmatrix} (-f_{h} \times \omega + v) \end{bmatrix}^{T}.$$
(43)

Note that ω_t is the rolling velocity of the head projected onto the tangent plane of the contact and v_t is the sliding velocity; ω_n is the relative rotational velocity projected to the contact's surface normal, and $\tilde{\mathcal{K}}_1 = R_\psi \mathcal{K}_1 R_\psi$ is the curvature of the IAB with respect to the contact frame that coincides with the normalized Gauss frame at $p_1(t)$. The matrix $(\mathcal{K}_h + \tilde{\mathcal{K}}_1)^{-1}$ is the so-called *relative curvature* originally coined by [24]. Simplifying (43), we find that

$$x_{h} = \frac{\partial f}{\partial u_{h}} / \| \frac{\partial f}{\partial u_{h}} \|, \quad y_{h} = \frac{\partial f}{\partial v_{h}} / \| \frac{\partial f}{\partial v_{h}} \|, \quad z_{h} = n_{u}(f(u))$$

$$T_{h} = y_{h} \left[\frac{\partial x_{h}^{T}}{\partial u_{h}} / \| \frac{\partial f}{\partial u_{h}} \|, \frac{\partial x_{h}^{T}}{\partial v_{h}} / \| \frac{\partial f}{\partial v_{h}} \| \right],$$

$$T_{1} = y_{1} \left[\frac{\partial x_{1}^{T}}{\partial u_{1}} / \| \frac{\partial f}{\partial u_{1}} \|, \frac{\partial x_{1}^{T}}{\partial v_{1}} / \| \frac{\partial f}{\partial v_{1}} \| \right],$$

$$\mathcal{K}_{h} = \left[x_{h}^{T}, \quad y_{h}^{T} \right]^{T} \left[\frac{\partial n_{h}^{T}}{\partial u_{h}} / \| \frac{\partial f}{\partial u_{h}} \|, \frac{\partial n_{h}^{T}}{\partial v_{h}} / \| \frac{\partial f}{\partial v_{h}} \| \right],$$

$$\mathcal{K}_{1} = \left[x_{1}^{T}, \quad y_{1}^{T} \right]^{T} \left[\frac{\partial n_{1}^{T}}{\partial u_{1}} / \| \frac{\partial f}{\partial u_{1}} \|, \frac{\partial n_{1}^{T}}{\partial v_{2}} / \| \frac{\partial f}{\partial v_{1}} \| \right]. \tag{44}$$

This is verified in Appendix C. We see that for the contact interaction between an IAB and the head, for a $U \subset \mathbb{R}^2$ we must choose an appropriate $f_i: U_i \to S_i \subset \mathbb{R}^3$ in order to characterize the setup.

V. MULTI-IAB STATICS AND END-EFFECTOR VELOCITIES

At a material point, \mathbf{r} , of the IAB surface in the configuration \mathcal{B} , the 3D position of a point is given by (6). Since deformation is radially symmetric, it follows that the regularity of the IAB in its current configuration, $\chi(\mathbf{r},t)$, implies that it can be uniformly defined by \mathbf{r} throughout the IAB material body. Similar to [3], we are interested in the final state of the IAB after deformation; the path it takes for us to reach the final configuration is not important to us (since there is no obstacle in the continuum robots' workspace). Thus we drop the time dependence on the configuration and take \mathbf{r} to be the generalized coordinate of the IAB. The configuration space of the IAB with respect to the spatial frame at a certain time can then be described by $g_{st}(\chi) \equiv g_{st}(\mathbf{r}) : \mathbf{r} \to g_{st}(\mathbf{r}) \in SE(3)$ while the strain state of the IAB is characterized by the strain field

$$\hat{\xi}_i(\mathbf{r}) = g_i^{-1} \frac{\partial g_i}{\partial \mathbf{r}} \in \mathfrak{se}(3) = g_i^{-1} g_i' \tag{45}$$

with the respective g_i' s being the tangent vector at g_i such that $g_i' \in T_{g_i(\mathbf{r})}SE(3)$. Note that $T_{g_i(\mathbf{r})}$ is the tangent matrix at g_i with associated Lie algebra $se(3) \approx T_eSE(3)$.

A. End Effector Forces

From the derived relationship between the head contact coordinates and the relative motion (v_t, ω_t) of the IAB i.e. equation (42), we can associate a Jacobian that maps IAB velocities to head position and orientation. A fundamental assumption in our formulation is that the IABs make contact with the head throughout manipulation, and the manipulation is stable and prehensile. A forward kinematic map from the configuration of the i'th IAB, χ_{iab_i} maps from respective IAB configurations to head position and orientation i.e. K_{iab_i} : $\chi_{iab_i} \rightarrow SE(3)$. The velocity of the head with respect to a fixed base frame in terms of IAB velocities can be written in terms of the forward kinematics Jacobian:

$$\begin{pmatrix} v_{iab_i} \\ \omega_{iab_i} \end{pmatrix} = \frac{\partial K_{iab_i}}{\partial \mathbf{r}_i} \frac{d\mathbf{r}}{dt} K_{iab_i}^{-1} = \mathbf{J}_i(\mathbf{r}_i) \dot{\mathbf{r}}_i$$
(46)

where \mathbf{r}_i is the spatial position of IAB i, and $(v_{iab_i}^T, \omega_{iab_i}^T) \in \mathbb{R}^6$ represents the linear and angular velocity of the i^{th} IAB about its screw basis. In essence, $\mathbf{r}_i \in \mathbb{R}^3$ with its rows of mapped to scalars by an appropriate choice of norm. The contact between the head and the IABs is mapped by the Jacobian

$$\boldsymbol{J}_{c_i}(\xi_h, \xi_{iab_i}) = \begin{bmatrix} \mathbf{I} & \hat{\boldsymbol{w}}(r_{c_i}) \\ \mathbf{0} & \mathbf{I} \end{bmatrix} J_{r_i}, \tag{47}$$

where $J_{c_i}: \dot{\xi}_{r_i} \to \begin{bmatrix} v_{c_i}^T, & w_{c_i}^T \end{bmatrix}^T$, $r_{c_i} \in \mathbb{R}^3$ is a vector between the head reference point (e.g. the center of mass) and the contact with the i^{th} IAB, ξ_h is the position and relative orientation of the head, ξ_{iab_i} is the position and relative orientation of the i^{th} soft robot in world coordinates,

 $\hat{w}(r_{c_i})$ is an anti-symmetric matrix for the vector r_{c_i} , and $\xi_r = (\xi_{r_1}, \xi_{r_2}, \cdots, \xi_{r_8})$ are the positions and orientations for each of the 8 IABs. The manipulation map, G_i is made up of matrices of the form

$$G_i(\xi_h, \xi_r) = \begin{bmatrix} \mathbf{I} & \mathbf{0} \\ \hat{w}(r_{c_i}) & \mathbf{I} \end{bmatrix} B_i(\xi_h, \xi_r), \tag{48}$$

where $B_i(\xi_h, \xi_r)$ is the selection map as defined in [22] for the desired manipulation. The net force on the head is a sum of the individual forces arising from each IAB. Owing to the linearity of each individual IAB's contact force, the resultant head force can be stitched together to form G, *i.e.*

$$\tilde{F}_h = \begin{bmatrix} G_1, \dots, G_8 \end{bmatrix} \begin{pmatrix} \tilde{F}_{c_1} \\ \vdots \\ \tilde{F}_{c_8} \end{pmatrix} = G\tilde{F}_c, \tag{49}$$

where $F_h \in \mathbb{R}^6$ and $F_c \in \mathbb{R}^{m_1} \times \mathbb{R}^{m_2} \times \ldots \times \mathbb{R}^{m_8}$. The *internal* or *null forces* is captured by the null space $\mathcal{N}(G)$ of the manipulation map G; these forces correspond to zero net force on the head of the patient. Each \tilde{F}_{c_i} in (49) is of the form (35).

B. End-effector Velocities

We define the velocity constraint dual of (48) as the constraint between the relative velocity of the head and that of the twist velocities of the contact point

$$\begin{pmatrix} \tilde{v}_{c_i} \\ \tilde{\omega}_{c_i} \end{pmatrix} = \begin{bmatrix} \mathbf{I} & \hat{\omega}(r_{c_i}) \\ 0 & \mathbf{I} \end{bmatrix} \begin{pmatrix} v_{c_h} \\ \omega_{c_h} \end{pmatrix}. \tag{50}$$

For a conjugate twist vector $(v_c^T, \omega_c^T)^T$ to the forces exerted by the IABs, f_c , we have the following

$$\begin{pmatrix} v_c \\ \omega_c \end{pmatrix} = G^T \begin{pmatrix} v_{c_h} \\ \omega_{c_h} \end{pmatrix}. \tag{51}$$

Given a selection matrix $B_i^T(\xi_h, \xi_{iab_i}) \in \mathbb{R}_i^m$ for a particular IAB, where m_i is the range of all the forces and moments for the chosen contact primitive (or union of contact primitives), the manipulation map for the i^{th} IAB can be written as,

$$G_i^T(\xi_h, \xi_{iab_i})\xi_h = B_i^T(\xi_h, \xi_{iab_i}) \boldsymbol{J}_{c_i}(\xi_h, \mathbf{r}_{r_i}) \dot{\xi}_{iab_i}$$
 (52)

where J_{c_i} is the contact Jacobian for the i^{th} actuator, and ξ_h denotes the velocity of the head. For the 8 soft actuators, the manipulation constraint of the system can be written as

$$\begin{bmatrix} G_1^T \\ G_2^T \\ \vdots \\ G_8^T \end{bmatrix} \begin{pmatrix} v_h \\ w_h \end{pmatrix} = \operatorname{diag} \begin{pmatrix} B_1^T \boldsymbol{J}_{c_1} \\ B_2^T \boldsymbol{J}_{c_2} \\ \vdots \\ B_8^T \boldsymbol{J}_{c_8} \end{pmatrix} \begin{pmatrix} \dot{\boldsymbol{r}}_{iab_1} \\ \dot{\boldsymbol{r}}_{iab_2} \\ \vdots \\ \dot{\boldsymbol{r}}_{iab_8} \end{pmatrix}. \quad (53)$$

VI. NEWTON-EULER SYSTEM OF EQUATIONS

The dynamics of the head is a form of (18) but without the actuator torques. In local coordinates, it has the form

$$\mathbf{M}_{h}(\zeta)\ddot{\zeta} + \mathbf{C}_{h}(\zeta,\dot{\zeta})\dot{\zeta} + \mathbf{N}_{h}(\zeta,\dot{\zeta}) = 0 \tag{54}$$

with ζ being a local parameterization of the position and orientation of the head in the Lie Group SE(3), and N_h being the gravitational and frictional forces exerted by/on the head.

The head and the multi-DOF IAB system are connected via the manipulation constraint i.e.

$$G^{T}(\zeta, \mathbf{r})\dot{\zeta} = J(\zeta, \mathbf{r})\dot{\mathbf{r}}.$$
 (55)

Suppose that the velocity constraint produces a virtual displacement constraint in $\delta \zeta$ and $\delta \mathbf{r}$ such that for $q=(\zeta,\mathbf{r})$, we have

$$\delta \mathbf{r} = \mathbf{J}^{-1}(q)G^T(q)\delta \zeta$$

the Lagrange equations become

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{q}} - \frac{\partial L}{\partial q} - (\tau, 0)\right)\delta q = 0 \quad (56a)$$

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \mathbf{r}} - \tau\right)^{T} \begin{pmatrix} \delta \mathbf{r} \\ \delta \zeta \end{pmatrix} = 0 \quad (56b)$$

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \zeta} - \frac{\partial L}{\partial \zeta}\right)^{T} \begin{pmatrix} \delta \mathbf{r} \\ \delta \zeta \end{pmatrix} = 0 \quad (56b)$$

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \mathbf{r}} - \tau\right)\delta \mathbf{r} + \left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\zeta}} - \frac{\partial L}{\partial \zeta}\right)\delta\zeta = 0 \quad (56c)$$

$$GJ^{-T} \left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \mathbf{r}} - \tau\right)\delta\zeta + \left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\zeta}} - \frac{\partial L}{\partial \zeta}\right)\delta\zeta = 0$$

wherefore.

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\zeta}} - \frac{\partial L}{\partial \zeta}\right)\delta\zeta + GJ^{-T}\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\mathbf{r}}} - \frac{\partial L}{\partial \mathbf{r}}\right) = GJ^{-T}\boldsymbol{\tau}$$
(57)

given the arbitrariness of $\delta\zeta$. Equations (57) alongside (55) completely describe the system dynamics. Putting (17) into (57), we have

$$\left(\frac{d}{dt}\frac{\partial L}{\partial \dot{\zeta}} - \frac{\partial L}{\partial \zeta}\right)\delta\zeta = GJ^{-T}\left(1 - \frac{\rho}{2\|\mathbf{r}\|^2}\right)\boldsymbol{\tau}.$$
 (58)

VII. CONCLUSIONS

We have presented the kinematic motion equations and the Lagrangian dynamics for the mechanism presented in our previous publication. It remains to demonstrate the working examples in closed-loop head motion control. In a follow-up paper to be released shortly, we show how these formulations are applied in real-time on the patient-IAB system.

APPENDIX A ROBOT-HEAD DYNAMICS

We now derive the overall dynamics for the elastic IAB in Eulerian form. Following (7), a point on the surface of the IAB has the following description

$$\mathbf{r} = \begin{bmatrix} \lambda \\ r \\ \phi \end{bmatrix} = \begin{bmatrix} r/R \\ (R_o^3 + r_i^3 - R_i^3)^{1/3} \\ \beta - \alpha \end{bmatrix}$$
 (59)

so that

$$\dot{\mathbf{r}} = \begin{bmatrix} \dot{\lambda}, & \dot{r}, & \dot{\phi} \end{bmatrix}^T = \begin{bmatrix} \dot{r}/R, & 3r_i^2 \dot{r}_i, & -\dot{\alpha} \end{bmatrix}^T$$
 (60)

which follows since $\dot{R}=\dot{\beta}=0$ in the reference configuration. Similarly, we find that $\ddot{\bf r}$ is given as

$$\ddot{\mathbf{r}} = \begin{bmatrix} \ddot{\lambda}, & \ddot{r}, & \ddot{\phi} \end{bmatrix}^T = \begin{bmatrix} \ddot{r}/R, & 6r_i \dot{r_i}^2 + 3r_i \ddot{r_i}, & -\ddot{\alpha} \end{bmatrix}^T$$
 (61)

Recall the kinetic energy form of a continuum body (§ III)

$$T = \frac{1}{2}\rho \mathbf{v}(\mathbf{r}, t) \cdot \mathbf{v}(\mathbf{r}, t) = \frac{1}{2}\rho ||\dot{\mathbf{r}}||^2.$$
 (62)

Given the incompressibility of the IAB material body, the material mass density is uniform throughout the body at a configuration so that the rate of change of the body mass, ρ , vanishes.

A. Case I: Cauchy Elastic IAB Material Skins

Suppose we choose a Cauchy Elastic material so that the constitutive equation that governs the Cauchy stress tensor, σ , is independent of the path of the deformation from the reference configuration but is solely a function of the state of deformation. Then, it follows that V=0. We have

$$T = \frac{1}{2}\rho ||\dot{\mathbf{r}}||^2 = \frac{1}{2}\rho \left(\dot{r}^2/R^2 + 9r_i^2\dot{r_i}^2 + \dot{\alpha}^2\right)^{1/2}, V = 0.$$
(63)

It follows that the Lagrangian is

$$L(\mathbf{r}, \dot{\mathbf{r}}) = \frac{1}{2} \rho ||\dot{\mathbf{r}}||^2 = \frac{1}{2} \rho \left(\dot{r}^2 / R^2 + 9r_i^2 \dot{r_i}^2 + \dot{\alpha}^2 \right)^{1/2}$$
 (64)

and the derivatives of the canonical momenta are

$$\frac{d}{dt}\frac{\partial L}{\partial \dot{r}} = \frac{d}{dt}\left(\frac{\rho \dot{r}}{2R^2 \|\mathbf{r}\|^2}\right) = \frac{\rho \ddot{r}}{2R^2 \|\mathbf{r}\|^2} - \frac{\rho \dot{r}}{R \|\mathbf{r}\|^2}$$
(65a)

$$\frac{d}{dt}\frac{\partial L}{\partial \dot{r}_i} = \frac{d}{dt}\left(\frac{9\rho r_i^4 \dot{r}_i}{2\|\mathbf{r}\|^2}\right) = \frac{18\rho r_i^3 \dot{r}_i}{\|\mathbf{r}\|^2} + \frac{9\rho r_i^4 \ddot{r}_i}{2\|\mathbf{r}\|^2}$$
(65b)

$$\frac{d}{dt}\frac{\partial L}{\partial \dot{\phi}} = \frac{d}{dt}\frac{\partial L}{\partial \dot{\alpha}} = \frac{d}{dt}\left(\frac{\rho \dot{\alpha}}{2\|\mathbf{r}\|^2}\right) = \frac{\rho \ddot{\alpha}}{2}$$
(65c)

with the following associated generalized forces

$$\frac{\partial L}{\partial \lambda} = \frac{\partial L}{\partial r} = 0$$
 and $\frac{\partial L}{\partial \phi} = \frac{\partial L}{\partial \phi} = 0$. (66a)

Recalling the Euler-Lagrange equation from (10), we may write the torque that governs the system dynamics as

$$\tau = \frac{\rho \ddot{r}}{2R^2 \|\mathbf{r}\|^2} - \frac{\rho \dot{r}}{R \|\mathbf{r}\|^2} + \frac{18\rho r_i^3 \dot{r}_i}{\|\mathbf{r}\|^2} + \frac{9\rho r_i^4 \ddot{r}_i}{2\|\mathbf{r}\|^2} + \frac{\rho \ddot{\alpha}}{2}$$
 (67)

or in matrix form

$$\tau = \frac{\rho}{\|\mathbf{r}\|^2} \begin{bmatrix} 1/2R^2 & 0 & 0\\ 0 & 9r_i^4/2 & 0\\ 0 & 0 & \|\mathbf{r}\|^2/2 \end{bmatrix} \begin{bmatrix} \ddot{r}\\ \ddot{r}_i\\ \ddot{\alpha} \end{bmatrix} + \frac{\rho}{\|\mathbf{r}\|^2} \begin{bmatrix} -1/R & 0 & 0\\ 0 & 18r_i^3 & 0\\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} \dot{r}\\ \dot{r}_i\\ \dot{\alpha} \end{bmatrix},$$
(68)

and written neatly as,

$$\frac{2\|\mathbf{r}\|^{2}}{\rho}\boldsymbol{\tau} = \underbrace{\begin{bmatrix} 1/R^{2} & 0 & 0\\ 0 & 9r_{i}^{4} & 0\\ 0 & 0 & \|\mathbf{r}\|^{2} \end{bmatrix}}_{M_{iab}} \ddot{\mathbf{r}} + \underbrace{\begin{bmatrix} -2/R & 0 & 0\\ 0 & 36r_{i}^{3} & 0\\ 0 & 0 & 0 \end{bmatrix}}_{C_{iab}} \ddot{\mathbf{r}}$$
(69)

B. Case II: Green Elastic IAB Material Skins

When the stress tensor depends on the strain, we have from (21), that

$$V(\mathbf{r}) = \mathbf{tr}(\mathbf{S}\dot{\mathbf{F}}). \tag{70}$$

The associated force on the head is now a function of the kinetic and potential energies so that we have

$$L(\mathbf{r}, \dot{\mathbf{r}}) = \frac{1}{2} \rho ||\dot{\mathbf{r}}||^2 + \mathbf{tr}(()\mathbf{S}\dot{\mathbf{F}})$$
$$= \frac{1}{2} \rho \left(\dot{r}^2 / R^2 + 9r_i^2 \dot{r_i}^2 + \dot{\alpha}^2\right)^{1/2} + \mathbf{tr}(\mathbf{S}\dot{\mathbf{F}}) \quad (71)$$

Solving for the derivatives of the kinetic and potential energy as before, we have, TO-DO: ... to be continued.

APPENDIX B

DERIVATION OF IAB-HEAD CONTACT KINEMATICS

Here, we formulate the contact kinematics between an IAB and the head in a fashion similar to the single finger soft contact type postulated in [26]. We note that an alternative derivation that is more concise can be found in [24].

A. Contact Coordinates and Gaussian Map

Following equations (37a), (37b), and 38, we write

$$R f_1(\alpha_1) + p = f_h(\alpha_h) \tag{72a}$$

$$R n_1(\alpha_1) = -n_h(\alpha_h) \tag{72b}$$

$$R\frac{\partial f_1}{\partial \alpha_1} M_1^{-1} R_{\psi} = \frac{\partial f_h}{\partial \alpha_h} M_h^{-1}. \tag{72c}$$

Differentiating (72a) and (72b), we find that

$$\dot{R}f_1(\alpha_1) + R\frac{\partial f_1}{\partial \alpha_1}\dot{\alpha_1} + \dot{p} = \frac{\partial f_h}{\partial \alpha_h}\dot{\alpha_h}$$
 (73)

$$\dot{R} n_1(\alpha_1) + R \frac{\partial n_1}{\partial \alpha_1} \dot{\alpha}_1 = -\frac{\partial n_h}{\partial \alpha_h} \dot{\alpha}_h. \tag{74}$$

It follows through the multiplication of (73) by $\frac{\partial f_h}{\partial \alpha_h}^T$ and putting α_h into (74), we have

$$\dot{R} n_1(\alpha_1) + R \frac{\partial n_1}{\partial \alpha_1} \dot{\alpha}_1 = -\frac{\partial n_h}{\partial \alpha_h} M_h^{-2} \frac{\partial f_h}{\partial \alpha_h}^T \left(\dot{R} f_1(\alpha_1) + R \frac{\partial f_1}{\partial \alpha_1} \dot{\alpha}_1 + \dot{p} \right). \quad (75)$$

Now, putting (72c) into (75) and rearranging, we find that

$$\left[R\frac{\partial n_1}{\partial \alpha_1} + \frac{\partial n_h}{\partial \alpha_h} M_h^{-2} \left(\frac{\partial f_h^T}{\partial \alpha_h} \frac{\partial f_h}{\partial \alpha_h}\right) M_h^{-1} R_{\psi} M_1\right] \dot{\alpha}_1$$

$$= -\dot{R} n_1 - \frac{\partial n_h}{\partial \alpha_h} M_h^{-2} \frac{\partial f_h}{\partial \alpha_h}^T \left(\dot{R} f_1(\alpha_1) + \dot{p}\right). \quad (76)$$

Multiplying throughout by $M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T$, we have on the left hand side of the above as.

$$M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T \left(R \frac{\partial n_1}{\partial \alpha_1} + \frac{\partial n_h}{\partial \alpha_h} M_h^{-1} R_{\psi} M_1 \right) \dot{\alpha}_1. \tag{77}$$

Since

$$M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T = \frac{\partial f_h}{\partial \alpha_h} M_h^{-1} = \left(R \frac{\partial f_1}{\partial \alpha_1} M_1^{-1} R_\psi \right)^T$$
$$= R_\psi M_1^{-T} \frac{\partial f_1}{\partial \alpha_1}^T R^T, \tag{78}$$

equation (77) becomes

$$\dot{\alpha}_{1} \left(R_{\psi} M_{1}^{-T} \frac{\partial f_{1}}{\partial \alpha_{1}}^{T} \frac{\partial n_{1}}{\partial \alpha_{1}} + M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \frac{\partial n_{h}}{\partial \alpha_{h}} M_{h}^{-1} R_{\psi} M_{1} \right) \\
= \left(R_{\psi} M_{1}^{-T} \frac{\partial f_{1}}{\partial \alpha_{1}}^{T} \frac{\partial n_{1}}{\partial \alpha_{1}} M_{1}^{-1} R_{\psi} + M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \frac{\partial n_{h}}{\partial \alpha_{h}} M_{h}^{-1} \right) \\
\times R_{\psi} M_{1} \dot{\alpha}_{1}. \tag{79}$$

Setting

$$\tilde{\mathcal{K}}_1 = R_{\psi} M_1^{-T} \frac{\partial f_1}{\partial \alpha_1}^T \frac{\partial n_1}{\partial \alpha_1} M_1^{-1} R_{\psi}$$

and

$$\mathcal{K}_h = M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T \frac{\partial n_h}{\partial \alpha_h} M_h^{-1},$$

it follows from (75) that

$$\left(\tilde{\mathcal{K}}_{1} + \mathcal{K}_{h}\right) R_{\psi} M_{1} \dot{\alpha}_{1} =$$

$$M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \left[-\dot{R} n_{1} - \frac{\partial n_{h}}{\partial \alpha_{h}} M_{h}^{-2} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \left(\dot{R} f_{1} + \dot{p} \right) \right]$$

$$= -M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \dot{R} n_{1} - \mathcal{K}_{h} M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \left(\dot{R} f_{1} + \dot{p} \right) \quad (80)$$

so that

$$\dot{\alpha}_{1} = \left(\tilde{\mathcal{K}}_{1} + \mathcal{K}_{h}\right)^{-1} R_{\psi} M_{1}^{-1} \times \left[\underbrace{-M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \dot{R} n_{1}}_{w_{t}} - \mathcal{K}_{h} \underbrace{M_{h}^{-T} \frac{\partial f_{h}}{\partial \alpha_{h}}^{T} \left(\dot{R} f_{1} + \dot{p}\right)}_{v_{t}}\right]$$
(81)

or

$$\dot{\alpha}_1 = \left(\tilde{\mathcal{K}}_1 + \mathcal{K}_h\right)^{-1} R_{\psi} M_1^{-1} (w_t - \mathcal{K}_h v_t). \tag{82}$$

Finding the generalized velocity of the head with respect to a single IAB deformation is tantamount to finding $(\hat{w},v)=\dot{g}\,g^{-1}$. Thus,

$$\omega_t = -M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T \left(\omega \times (R \, n_1) \right) = -M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T \left(n_h \times \omega \right)$$
(83)

$$v_t = M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T \left(\omega \times (R f_1) + \omega \times p + v \right)$$
 (84)

$$= M_h^{-T} \frac{\partial f_h}{\partial \alpha_h}^T (-f_h \times \omega + v), \tag{85}$$

where ω_t is the head's rolling velocity projected onto the contact's tangent plane. The rotation normal to the surface is canceled by the cross product of ω and n_h . In the same vein, v_t is the sliding velocity between the contacts, projected onto the tangent plane. Following the above construction, we

find the kinematics of the contact point of the head in local coordinates is

$$\dot{\alpha}_h = M_h^{-1} \left(\tilde{\mathcal{K}}_1 + \mathcal{K}_h \right)^{-1} (\omega_t - \tilde{\mathcal{K}}_1 v_t), \tag{86}$$

where $(\tilde{\mathcal{K}}_1 + \mathcal{K}_h)$ is the *relative curvature* [24]. It remains to solve for the relative orientation between the two local coordinates, ψ .

B. Relative Contact Orientation and Torsion Metric Tensors
In matrix form, (72b) and (72c) can be written as,

$$R\begin{bmatrix} \frac{\partial f_1}{\partial \alpha_1} M_1^{-1} & n_1(\alpha_1) \end{bmatrix} \begin{bmatrix} R_{\psi} & 0 \\ 0 & -1 \end{bmatrix} = \begin{bmatrix} \frac{\partial f_h}{\partial \alpha_h} M_h^{-1} & n_h(\alpha_h) \end{bmatrix}.$$
(87)

Following the normalized Gaussian frame defined in (41), we can rewrite the above equation as

$$R[x_1 y_1 z_1] \bar{R}_{\psi} = [x_h y_h z_h]. \tag{88}$$

The total derivative of (88) yields

$$\dot{R} \begin{bmatrix} x_1 & y_1 & z_1 \end{bmatrix} \bar{R}_{\psi} + R \begin{bmatrix} \dot{x}_1 & \dot{y}_1 & \dot{z}_1 \end{bmatrix} \bar{R}_{\psi} + R \begin{bmatrix} x_1 & y_1 & z_1 \end{bmatrix} \begin{bmatrix} \dot{R}_{\psi} & 0 \\ 0 & 0 \end{bmatrix} = \begin{bmatrix} \dot{x}_h \\ \dot{y}_h \\ \dot{z}_t \end{bmatrix}^T . (89)$$

Premultiplying by $y_1^TR^T$ and then postmultiplying by $\bar{R}_{\psi}\begin{pmatrix} 1 \\ 0 \\ 0 \end{pmatrix}$, with the knowledge that $\bar{R}_{\psi}\bar{R}_{\psi}=\mathbf{I}$, and the identity $y_1^Ty_1=1$, we find that

$$y_{1}^{T}R^{T}\dot{R}[x_{1}\ y_{1}\ z_{1}]\bar{R}_{\psi} + y_{1}^{T}[\dot{x}_{1},\ \dot{y}_{1},\ \dot{z}_{1}]\bar{R}_{\psi} + (0\ 1\ 0)\begin{bmatrix}\dot{R}_{\psi} & 0\\ 0 & 0\end{bmatrix} = y_{1}^{T}R^{T}[\dot{x}_{h}\ \dot{y}_{h}\ \dot{z}_{h}]$$
(90)
$$y_{1}^{T}R^{T}\dot{R}x_{1} + y_{1}^{T}\dot{x}_{1} + (0\ 1\ 0)\begin{bmatrix}\dot{R}_{\psi}\ R_{\psi} & 0\\ 0 & 0\end{bmatrix}\begin{pmatrix}1\\0\\0\end{pmatrix}$$
(91)
$$= y_{1}^{T}R^{T}[\dot{x}_{h}\ \dot{y}_{h}\ \dot{z}_{h}]\bar{R}_{\psi}\begin{pmatrix}1\\0\\0\end{pmatrix}$$
(91)
$$= y_{1}^{T}R^{T}[\dot{x}_{h}\ \dot{y}_{h}\ \dot{z}_{h}]\bar{R}_{\psi}\begin{pmatrix}1\\0\\0\end{pmatrix}$$
(92)

$$y_1^T R^T \dot{R} x_1 + y_1^T \dot{x}_1 - \dot{\psi} = y_1^T R^T [\dot{x}_h \ \dot{y}_h \ \dot{z}_h] \bar{R}_{\psi} \begin{pmatrix} 1 \\ 0 \\ 0 \end{pmatrix}.$$
(93)

From (88), we have that

$$\bar{R}_{\psi}^{T} \begin{bmatrix} x_1^T & y_1^T & z_1^T \end{bmatrix} R^T = \begin{bmatrix} x_h^T & y_h^T & z_h^T \end{bmatrix}$$
 (94)

so that

$$\begin{bmatrix} x_1^T & y_1^T & z_1^T \end{bmatrix} R^T = \bar{R}_{\psi} \begin{bmatrix} x_h^T & y_h^T & z_h^T \end{bmatrix}$$
 (95)

or

$$y_1^T R^T = (0 \ 1 \ 0) \, \bar{R}_{\psi} \left[x_h^T \quad y_h^T \quad z_h^T \right]$$

$$= (0 \ 1) \, R_{\psi} \left(\begin{array}{c} x_h^T \\ y_h^T \end{array} \right).$$
(96)

It follows from (93) that

$$\dot{\psi} = y_1^T R^T \dot{R} x_1 + y_1^T \frac{\partial x_1}{\partial \alpha_1} \dot{\alpha}_1 - (0, 1) R_{\psi} \begin{bmatrix} x_h^T \dot{x}_h & x_h^T \dot{y}_h \\ y_h^T \dot{x}_h & y_h^T \dot{y}_h \end{bmatrix} R_{\psi} \begin{pmatrix} 1 \\ 0 \end{pmatrix}.$$
 (97)

Using the identities,

$$x_i^T y_i = 0, \implies \dot{x}_i^T y_i = -x_i^T \dot{y}_i = y_i^T \dot{x}_i$$

$$x_i^T x_i = 1, \implies \dot{x}_i^T x_i = 0.$$

$$(98)$$

we can rewrite (97) as

$$\dot{\psi} = y_1^T R^T \dot{R} x_1 + y_h^T \frac{\partial x_h}{\partial \alpha_h} \dot{\alpha}_h + y_1^T \frac{\partial x_1}{\partial \alpha_1} \dot{\alpha}_1$$

$$= \omega_n + T_h M_h \dot{\alpha}_h + T_1 M_1 \dot{\alpha}_1 \tag{100}$$

where

$$\omega_n = y_1^T R^T \dot{R} x_1 = (R y_1)^T w \times (R x_1)$$

= $(R z_1)^T \omega = z_h^T \omega$ (101)

$$T_h = y_h \frac{\partial x_h^T}{\partial \alpha_h} M_h^{-T}, \qquad T_1 = y_1 \frac{\partial x_1^T}{\partial \alpha_1} M_1^{-T}.$$
 (102)

It follows that the first, second and third equations of contact are given by (82), (86), and (100) respectively, *i.e.*

Equations of Contact

$$\dot{\alpha}_1 = \left(\tilde{\mathcal{K}}_1 + \mathcal{K}_h\right)^{-1} R_{\psi} M_1^{-1} (\omega_t - \mathcal{K}_h v_t) \quad \text{(103a)}$$

$$\dot{\alpha}_h = M_h^{-1} \left(\tilde{\mathcal{K}}_1 + \mathcal{K}_h \right)^{-1} \left(\omega_t - \tilde{\mathcal{K}}_1 v_t \right) \tag{103b}$$

$$\dot{\psi} = \omega_n + T_h M_h \dot{\alpha}_h + T_1 M_1 \dot{\alpha}_1. \tag{103c}$$

APPENDIX C BASE IAB-HEAD BOUNDARY VALUE PROBLEM

In general, we expect that the 2-IAB chains will preserve spherically symmetric deformation since the side force from the object is minimal. Again, the spherical deformation principle is a first order approximation to aid a simplified model. For the base IABs in the closed kinematic chain, it is natural to expect the the IABs to be deformed anisotropically. In this appendix, we derive the kinematics that governs such deformations. The kinematics for the side IAB chains holds from equations 24-27 of [3].

With the spherically symmetric deformation property, we expect that the shear stress contributions $\sigma_{r\phi}$, $\sigma_{r\theta}$, $\sigma_{\phi\theta}$ vanish

in the body forces equation so that we have from the equation of balance of linear momentum,

$$\frac{1}{r^2} \frac{\partial}{\partial r} (r^2 \sigma_{rr}) - \frac{1}{r} (\sigma_{\theta\theta} + \sigma_{\phi\phi}) + \rho b_r = \rho \ddot{\mathbf{r}}_x \qquad (104a)$$

$$\frac{1}{r \sin \phi} \frac{\partial}{\partial \phi} (\sin \phi \sigma_{\phi\phi}) - \frac{\cot \phi}{r} (\sigma_{\theta\theta}) + \rho b_{\phi} = \rho \ddot{\mathbf{r}}_y \qquad (104b)$$

$$\frac{1}{r \sin \phi} \frac{\partial}{\partial \theta} (\sigma_{\theta\theta}) + \rho b_{\theta} = \rho \ddot{\mathbf{r}}_z \qquad (104c)$$

where the mass density ρ is uniform throughout the body and the components $\ddot{\mathbf{r}}_x, \ddot{\mathbf{r}}_y$, and $\ddot{\mathbf{r}}_z$ are as given in (65). Solving the equations in (104), we have from (104a),

$$\frac{\partial \sigma_{rr}}{\partial r} = \rho \ddot{\mathbf{r}}_x + \frac{1}{r} (\sigma_{\theta\theta} + \sigma_{\phi\phi}) - \rho b_r
= \frac{1}{r} (\sigma_{\theta\theta} + \sigma_{\phi\phi}) - \rho b_r
+ \rho \cos \theta \left(2\dot{r}\dot{\phi}\cos \theta + r\cos \theta \ddot{\phi} - 2r\dot{\theta}\dot{\phi}\sin \theta \right)
- \rho \sin \phi \left(\cos \theta (-\ddot{r} + r\dot{\theta}^2 + r\dot{\phi}^2) + \sin \theta (2\dot{r}\dot{\theta} + r\ddot{\theta}) \right)$$
(105)

and from (104b), we have

$$\begin{split} \rho \ddot{\mathbf{r}}_y &= \frac{\cot \phi}{r} (\sigma_{\phi\phi} - \sigma_{\theta\theta}) + \rho b_\phi + \frac{1}{r} \frac{\partial \sigma_{\phi\phi}}{\partial \phi} \\ \frac{\partial \sigma_{\phi\phi}}{\partial \phi} &= r \rho \ddot{\mathbf{r}}_y - r \rho b_\phi. \end{split}$$

so that

$$\frac{\partial \sigma_{\phi\phi}}{\partial \phi} = -\rho r b_{\theta} + r \rho \left[\cos \phi \left(2r \dot{\theta} \dot{\phi} \cos \theta + (2\dot{r} \dot{\phi} + r \ddot{\phi}) \sin \theta \right) + \sin \theta \left(2\dot{r} \dot{\theta} \cos \theta + r \ddot{\theta} \cos \theta + (\ddot{r} - r \dot{\theta}^2 - r \dot{\phi}^2) \right) \sin \phi \right]$$
(106)

and lastly, we have from (104c)

$$\frac{\partial \sigma_{\theta\theta}}{\partial \theta} = (\rho \ddot{\mathbf{r}}_z - \rho b_\theta) r \sin \phi$$

$$= -r \rho b_\theta \sin \phi + r \rho \sin \phi \cos \phi \left(\ddot{r} - r \dot{\phi}^2 \right)$$

$$- r \rho \sin^2 \phi \left(2 \dot{r} \dot{\phi} + r \ddot{\phi} \right). \tag{107}$$

Collecting $\frac{\partial \sigma_{rr}}{\partial r}$, $\frac{\partial \sigma_{\theta\theta}}{\partial \theta}$, and $\frac{\partial \sigma_{\phi\phi}}{\partial \phi}$ above, taking $\sigma_{rr}(r_{\circ}) = \sigma_{\theta\theta}(2\pi) = \sigma_{\phi\phi}(\pi) = 0$ and integrating from the internal to outer boundary conditions given by

$$\sigma_{rr}|_{R=R_o} = -P_{\text{atm}}, \quad \sigma_{rr}|_{R=R_i} = -P_{\text{atm}} - P$$
 (108)

we have the full form of the normal stress components as

$$\sigma_{rr}(\delta) = -\int_{\delta}^{r_{\circ}} \left[\frac{1}{r} \left(-2p + 2C_{1} \frac{r^{2}}{R^{2}} - 2C_{2} \frac{R^{8}}{r^{8}} \right) - \rho b_{r} \right]$$

$$+ \rho \cos \theta \left(2\dot{r}\dot{\phi}\cos\theta + r\cos\theta\ddot{\phi} - 2r\dot{\theta}\dot{\phi}\sin\theta \right)$$

$$-\rho \sin \phi \left(\cos\theta(-\ddot{r} + r\dot{\theta}^{2} + r\dot{\phi}^{2}) + \sin\theta(2\dot{r}\dot{\theta} + r\ddot{\theta}) \right) \right] dr,$$

$$\sigma_{\phi\phi}(\epsilon) = -\int_{\epsilon}^{\pi} \left[r\rho \left[\cos\phi \left(2r\dot{\theta}\dot{\phi}\cos\theta + (2\dot{r}\dot{\phi} + r\ddot{\phi})\sin\theta \right) + \right. \right]$$

$$\sin\theta \sin\phi \left(2\dot{r}\dot{\theta}\cos\theta + r\ddot{\theta}\cos\theta + (\ddot{r} - r\dot{\theta}^{2} - r\dot{\phi}^{2}) \right) \right]$$

$$-\rho rb_{\theta} d\phi$$

$$\sigma_{\theta\theta}(\zeta) = -\int_{\zeta}^{2\pi} \left[-r\rho b_{\theta} \sin\phi + r\rho \sin\phi \cos\phi \left(\ddot{r} - r\dot{\phi}^{2} \right) - r\rho \sin^{2}\phi \left(2\dot{r}\dot{\phi} + r\ddot{\phi} \right) \right] d\theta \qquad (110)$$

where $r_i \leq \delta \leq r_o$, $0 \leq \epsilon \leq \pi$ and $0 \leq \zeta \leq 2\pi$. Now, using the boundary condition, $P + P_{\text{atm}} = -\sigma_{rr}|_{r=r_i}$, where P_{atm} is the atmospheric pressure, (here, taken as 0), we have the internal pressure in the IAB cavity as a function of the radius of deformation in the current configuration as

$$P = \int_{r_i}^{r_0} \left[\frac{1}{r} \left(-2p + 2C_1 \frac{r^2}{R^2} - 2C_2 \frac{R^8}{r^8} \right) - \rho b_r \right.$$
$$\left. + \rho \cos \theta \left(2\dot{r}\dot{\phi}\cos\theta + r\cos\theta\ddot{\phi} - 2r\dot{\theta}\dot{\phi}\sin\theta \right) \right.$$
$$\left. - \rho \sin \phi \left(\cos\theta(-\ddot{r} + r\dot{\theta}^2 + r\dot{\phi}^2) + \sin\theta(2\dot{r}\dot{\theta} + r\ddot{\theta}) \right) \right] dr.$$
(111)

ACKNOWLEDGMENT

The author would like to thank Erik Pearson for kindly providing the CAD models of the couch and gantry used in the SOFA model.

REFERENCES

- U.S. Department of Health and Human Services, National Institutes of Health, National Cancer Institute. (2019) Cancer Stat Facts: Cancer of Any Site. [Online]. Available: https://seer.cancer.gov/statfacts/html/all.html
- [2] M. D. Michaelson, S. E. Cotter, P. C. Gargollo, A. L. Zietman, D. M. Dahl, and M. R. Smith, "Management of complications of prostate cancer treatment," *CA: a cancer journal for clinicians*, vol. 58, no. 4, pp. 196–213, 2008.
- [3] O. Ogunmolu, X. Liu, and R. Wiersma, "Mechanism and Constitutive Model of a Continuum Robot for Head and Neck Cancer Radiotherapy," 2019. 1, 2, 4, 5, 7, 10
- [4] O. P. Ogunmolu, "A Multi-DOF Soft Robot Mechanism for Patient Motion Correction and Beam Orientation Selection in Cancer Radiation Therapy." Ph.D. dissertation, The University of Texas at Dallas; UT Southwestern Medical Center, 2019.
- [5] J. M. Bern, K.-H. Chang, and S. Coros, "Interactive design of animated plushies," ACM Transactions on Graphics (TOG), vol. 36, no. 4, p. 80, 2017.
- [6] J. M. Bern, G. Kumagai, and S. Coros, "Fabrication, modeling, and control of plush robots," in 2017 IEEE/RSJ International Conference on Intelligent Robots and Systems (IROS). IEEE, 2017, pp. 3739–3746.
- [7] T. Liu, S. Bouaziz, and L. Kavan, "Quasi-newton methods for real-time simulation of hyperelastic materials," ACM Transactions on Graphics (TOG), vol. 36, no. 3, p. 23, 2017.
- [8] S. Bouaziz, S. Martin, T. Liu, L. Kavan, and M. Pauly, "Projective dynamics: fusing constraint projections for fast simulation," ACM Transactions on Graphics (TOG), vol. 33, no. 4, p. 154, 2014.
- [9] M. Giorelli, F. Renda, M. Calisti, A. Arienti, G. Ferri, and C. Laschi, "Neural Network And Jacobian Method For Solving The Inverse Statics Of A Cable-driven Soft Arm With Nonconstant Curvature," *IEEE Transactions on Robotics*, vol. 31, no. 4, pp. 823–834, 2015.
- [10] O. Ogunmolu, A. Kulkarni, Y. Tadesse, X. Gu, S. Jiang, and N. Gans, "Soft-neuroadapt: A 3-dof neuro-adaptive patient pose correction system for frameless and maskless cancer radiotherapy," in *IEEE/RSJ Interna*tional Conference on Intelligent Robots and Systems (IROS), Vancouver, BC, CA. IEEE, 2017, pp. 3661–3668. 1
- [11] H. Mochiyama, "Hyper-flexible robotic manipulators," in *IEEE International Symposium on Micro-NanoMechatronics and Human Science*, 2005. IEEE, 2005, pp. 41–46. 1
- [12] G. S. Chirikjian and J. W. Burdick, "The kinematics of hyper-redundant robot locomotion," *IEEE transactions on robotics and automation*, vol. 11, no. 6, pp. 781–793, 1995.

- [13] F. Renda and L. Seneviratne, "A Geometric and Unified Approach for Modeling Soft-Rigid Multi-body Systems with Lumped and Distributed Degrees of Freedom," 2018 IEEE International Conference on Robotics and Automation (ICRA), pp. 1567 – 1574, 2018.
- [14] H. Demirkoparan and T. J. Pence, "Swelling of an Internally Pressurized Nonlinearly Elastic Tube with Fiber Reinforcing," *International journal* of solids and structures, vol. 44, no. 11-12, pp. 4009–4029, 2007. 1
- [15] A. Sedal, D. Bruder, J. Bishop-Moser, R. Vasudevan, and S. Kota, "A continuum model for fiber-reinforced soft robot actuators," *Journal of Mechanisms and Robotics*, vol. 10, no. 2, p. 024501, 2018.
- [16] T. George Thuruthel, Y. Ansari, E. Falotico, and C. Laschi, "Control Strategies for Soft Robotic Manipulators: A Survey," *Soft Robotics*, vol. 5, no. 2, pp. 149–163, 2018.
- [17] O. Ogunmolu, N. Gans, S. Jiang, and X. Gu, "An Image Guided Soft Robotic Patient Positioning System for Maskless Head And Neck Cancer Radiotherapy: A Proof of Concept Study," *Medical Physics: The International Journal of Medical Physics Research and Practice*, vol. 42, pp. 3266–3266, June 2015. 1
- [18] O. P. Ogunmolu, X. Gu, S. Jiang, and N. R. Gans, "A real-time, soft robotic patient positioning system for maskless head-and-neck cancer radiotherapy: An initial investigation," in *Automation Science and Engi*neering (CASE), 2015 IEEE International Conference on, Gothenburg, Sweden. IEEE, 2015, pp. 1539–1545. 1
- [19] O. P. Ogunmolu, X. Gu, S. Jiang, and N. R. Gans, "Vision-based control of a soft robot for maskless head and neck cancer radiotherapy," in Automation Science and Engineering (CASE), 2016 IEEE International Conference on, Fort Worth, Texas. IEEE, 2016, pp. 180–187.
- [20] R. Ogden, Non-linear Elastic Deformations. Mineola, New York: Dover Publicationbs, Inc., 1997. 1, 3, 4, 5
- [21] C. Truesdell and W. Noll, The Non-Linear Field Theories of Mechanics. Springer, 1965.
- [22] J. R. Kerr, "An Analysis of Multi-Fingered Hands," *International Journal of Robotics Research*, no. Dept. of Mechanical Engineering, pp. 3–17, 1984. 7
- [23] V.-D. Nguyen, "Constructing force-closure grasps," *The International Journal of Robotics Research*, vol. 7, no. 3, pp. 3–16, 1988. 4
- [24] D. J. Montana, "The Kinematics of Contact And Grasp," The International Journal of Robotics Research, vol. 7, no. 3, pp. 17–32, 1988. 4, 6, 9, 10
- [25] M. Spivak, "A Comprehensive Introduction to Differential Geometry. Vol. V. Berkeley: Publish or Perish," *Inc. XI*, 1979. 6
- [26] R. M. Murray and S. Sastry, "Grasping and Manipulation using Multi-fingered Robot Hands." in *Proceedings of Symposia in Applied Mathematics*, vol. 41, 1990, pp. 329–335. 6, 9