



UNIVERSITÀ DEGLI STUDI DI PADOVA

Dipartimento di Scienze Statistiche

Corso di Dottorato di Ricerca in Scienze Statistiche

Ciclo XXXIV

THESIS TITLE

Coordinatore del Corso: Prof. Nicola Sartori

Supervisore: Prof. Antonio Canale

Co-supervisore: Prof. Michele Guindani

Dottoranda: Laura D'Angelo

giorno mese 2021

ABSTRACT

Lorem ipsum dolor sit amet, consectetur adipiscing elit. Ut purus elit, vestibulum ut, placerat ac, adipiscing vitae, felis. Curabitur dictum gravida mauris. Nam arcu libero, nonummy eget, consectetur id, vulputate a, magna. Donec vehicula augue eu neque. Pellentesque habitant morbi tristique senectus et netus et malesuada fames ac turpis egestas. Mauris ut leo. Cras viverra metus rhoncus sem. Nulla et lectus vestibulum urna fringilla ultrices. Phasellus eu tellus sit amet tortor gravida placerat. Integer sapien est, iaculis in, pretium quis, viverra ac, nunc. Praesent eget sem vel leo ultrices bibendum. Aenean faucibus. Morbi dolor nulla, malesuada eu, pulvinar at, mollis ac, nulla. Curabitur auctor semper nulla. Donec varius orci eget risus. Duis nibh mi, congue eu, accumsan eleifend, sagittis quis, diam. Duis eget orci sit amet orci dignissim rutrum.

Nam dui ligula, fringilla a, euismod sodales, sollicitudin vel, wisi. Morbi auctor lorem non justo. Nam lacus libero, pretium at, lobortis vitae, ultricies et, tellus. Donec aliquet, tortor sed accumsan bibendum, erat ligula aliquet magna, vitae ornare odio metus a mi. Morbi ac orci et nisl hendrerit mollis. Suspendisse ut massa. Cras nec ante. Pellentesque a nulla. Cum sociis natoque penatibus et magnis dis parturient montes, nascetur ridiculus mus. Aliquam tincidunt urna. Nulla ullamcorper vestibulum turpis. Pellentesque cursus luctus mauris.

SOMMARIO

Lorem ipsum dolor sit amet, consectetur adipiscing elit. Ut purus elit, vestibulum ut, placerat ac, adipiscing vitae, felis. Curabitur dictum gravida mauris. Nam arcu libero, nonummy eget, consectetur id, vulputate a, magna. Donec vehicula augue eu neque. Pellentesque habitant morbi tristique senectus et netus et malesuada fames ac turpis egestas. Mauris ut leo. Cras viverra metus rhoncus sem. Nulla et lectus vestibulum urna fringilla ultrices. Phasellus eu tellus sit amet tortor gravida placerat. Integer sapien est, iaculis in, pretium quis, viverra ac, nunc. Praesent eget sem vel leo ultrices bibendum. Aenean faucibus. Morbi dolor nulla, malesuada eu, pulvinar at, mollis ac, nulla. Curabitur auctor semper nulla. Donec varius orci eget risus. Duis nibh mi, congue eu, accumsan eleifend, sagittis quis, diam. Duis eget orci sit amet orci dignissim rutrum.

Nam dui ligula, fringilla a, euismod sodales, sollicitudin vel, wisi. Morbi auctor lorem non justo. Nam lacus libero, pretium at, lobortis vitae, ultricies et, tellus. Donec aliquet, tortor sed accumsan bibendum, erat ligula aliquet magna, vitae ornare odio metus a mi. Morbi ac orci et nisl hendrerit mollis. Suspendisse ut massa. Cras nec ante. Pellentesque a nulla. Cum sociis natoque penatibus et magnis dis parturient montes, nascetur ridiculus mus. Aliquam tincidunt urna. Nulla ullamcorper vestibulum turpis. Pellentesque cursus luctus mauris.

Nulla malesuada porttitor diam. Donec felis erat, congue non, volutpat at, tincidunt tristique, libero. Vivamus viverra fermentum felis. Donec nonummy pellentesque ante. Phasellus adipiscing semper elit. Proin fermentum massa ac quam. Sed diam turpis, molestie vitae, placerat a, molestie nec, leo. Maecenas lacinia. Nam ipsum ligula, eleifend at, accumsan nec, suscipit a, ipsum. Morbi blandit ligula feugiat magna. Nunc eleifend consequat lorem. Sed lacinia nulla vitae enim. Pellentesque tincidunt purus vel magna. Integer non enim. Praesent euismod nunc eu purus. Donec bibendum quam in tellus. Nullam cursus pulvinar lectus. Donec et mi. Nam vulputate metus eu enim. Vestibulum pellentesque felis eu massa.

CONTENTS

INTRODUCTION	1
1 BACKGROUND: STATISTICAL MODELING OF CALCIUM IMAGING DATA	3
1.1 Overview of calcium imaging data	3
1.1.1 Deconvolution methods	3
1.1.2 Spike train data analysis	5
1.2 Data sets	5
1.2.1 Allen Brain Observatory data	5
1.2.2 Altri dati?	7
1.3 A brief review of some Bayesian nonparametric models	7
1.3.1 Finite mixture models	7
1.3.2 Dirichlet process mixture models	9
1.3.3 Mixtures of finite mixtures	13
1.3.4 Bayesian nonparametric models for nested data	16
2 EFFICIENT POSTERIOR SAMPLING FOR BAYESIAN POISSON REGRESSION	21
2.1 Efficient posterior sampling strategies	23
2.1.1 Approximate posterior distribution	23
2.1.2 Metropolis-Hastings sampler	24
2.1.3 Adaptive importance sampler	25
2.1.4 Tuning parameters r_i	25
2.2 Numerical illustrations	26
2.2.1 Synthetic data	26
2.2.2 Spike train data	29
3 DECONVOLUTION AND MODELING OF CALCIUM IMAGING DATA WITH DISCRETE STIMULUS	31
3.1 Model and prior specification	32
3.2 Posterior inference	34
3.3 Simulation study	35
3.4 Allen Brain Observatory data analysis	39
CONCLUSIONS	45
A APPENDIX NAME	47
BIBLIOGRAPHY	49

LIST OF FIGURES

1.1	Allen Brain Observatory data: calcium traces of two neurons located in the primary visual area during Session A and Session B of the experiment.	6
2.1	Time per independent sample for the importance sampler, MH and HMC algorithms. For each combination of n and p the boxplots represent the distribution of the time over the effective sample size using a Gaussian prior.	27
2.2	Time per independent sample for the importance sampler, MH and HMC algorithms. For each combination of n and p the boxplots represent the distribution of the time over the effective sample size using a horseshoe prior.	28
2.3	Coefficients of the regression on the calcium imaging data set: posterior density, with the posterior mean and 95% credible interval	29
3.1	Distribution of the misclassification error rate in the simulation study for the four considered methods: CAM, fCAM, and the methods of Jewell <i>et al.</i> (2019) “L0” and Friedrich <i>et al.</i> (2017) “L1”.	38
3.2	Distribution of the adjusted Rand index on the distributional and observational clusters, computed on the 50 simulations for the three scenarios of the simulated data.	39
3.3	Observed fluorescence trace y_t from the Allen Brain Observatory data (black line), and visual stimulus to which the mouse is exposed (shaded areas). The yellow line represents the estimated neuronal activity. . . .	40
3.4	Empirical distribution of the posterior means of the observational cluster parameters A_t for the three experimental conditions of the Allen Brain Observatory data.	41
3.5	Short interval of length 500 of the Allen Brain Observatory data in correspondence of a spike, for the three stimuli. The vertical lines indicate the time of a spike and the colors correspond to the observational cluster of its amplitude. The bottom panels show the estimated posterior probability of spike presence, for each time point.	43

LIST OF TABLES

INTRODUCTION

OVERVIEW

A fundamental but unsolved problem in neuroscience is understanding the functioning of neurons and neuronal networks in processing sensory information, generating locomotion, and mediating learning and memory. The investigation of the structure and function of the nervous system can be dated back to the nineteenth century with the invention of the technique of silver impregnation by Camillo Golgi in 1873, which allowed the visualization of individual neurons (Drouin *et al.*, 2015). The technique initiated the study of the microscopic anatomy of the nervous system, and the investigation of how neurons organize to form the brain. Ever since there has been a significant research effort both to discover the cellular properties of the nervous system, and to characterize behaviors and correlate them with activity imaged in different regions of the brain. However, many scientists recognize that despite the innovative techniques developed to observe and analyze neurons, we are still facing an “explanatory gap” between the understanding of elemental components and the outputs that they produce (Parker, 2006, 2010; Dudai, 2004). That is, we know a lot about the components of the nervous system, but still we have little insight into how these components work together to enable us to think, remember, or behave. One of the reasons of this gap is the availability of a huge quantity of data, but a lack of tools to integrate these data in order to obtain a coherent picture of the brain functioning (Parker, 2010).

The technological developments of the last few decades have opened fundamentally new opportunities to investigate the nervous system. Large neuronal networks can now be visualized using *in vivo* high-resolution imaging techniques, which permit to record the neuronal activity in freely moving animals over long periods of time. In this thesis, we focus on data resulting from the application of the two-photon calcium imaging technique. Calcium ions generate intracellular signals that determine a large variety of functions in all neurons: when a neuron fires, calcium floods the cell and produces a transient spike in its concentration (Grienberger and Konnerth, 2012). By using genetically encoded calcium indicators, which are fluorescent molecules that react when binding to the calcium ions, it is possible to optically measure the level of calcium by analyzing the observed fluorescence trace. However, extracting these fluorescent calcium traces is just the first step towards the understanding of brain circuits: how to relate the observed pattern of neuronal activity with its output remains an open problem of research.

MAIN CONTRIBUTIONS OF THE THESIS

Lorem ipsum dolor sit amet, consectetur adipiscing elit. Ut purus elit, vestibulum ut, placerat ac, adipiscing vitae, felis. Curabitur dictum gravida mauris. Nam arcu libero, nonummy eget, consectetur id, vulputate a, magna. Donec vehicula augue eu neque. Pellentesque habitant morbi tristique senectus et netus et malesuada fames ac turpis egestas. Mauris ut leo. Cras viverra metus rhoncus sem. Nulla et lectus vestibulum urna fringilla ultrices. Phasellus eu tellus sit amet tortor gravida placerat. Integer sapien est, iaculis in, pretium quis, viverra ac, nunc. Praesent eget sem vel leo ultrices bibendum. Aenean faucibus. Morbi dolor nulla, malesuada eu, pulvinar at, mollis ac, nulla. Curabitur auctor semper nulla. Donec varius orci eget risus. Duis nibh mi, congue eu, accumsan eleifend, sagittis quis, diam. Duis eget orci sit amet orci dignissim rutrum.

1 | BACKGROUND: STATISTICAL MODELING OF CALCIUM IMAGING DATA

1.1. OVERVIEW OF CALCIUM IMAGING DATA

Calcium ions generate intracellular signals that control key functions in all types of neurons. At rest, most neurons have an intracellular calcium concentration of about 100 nM; however, during electrical activity, the concentration can rise transiently up to levels around 1000 nM (Berridge *et al.*, 2000). The development of techniques that enable the visualization and quantitative estimation of the intracellular calcium signals have thus greatly enhanced the investigation of neuronal functioning. The development of calcium imaging techniques involved two parallel processes: the development of calcium indicators, which are fluorescent molecules that react when binding to the calcium ions, and the implementation of the appropriate imaging instrumentation, in particular, the introduction of two-photon microscopy (Denk *et al.*, 1990). In recent years, the innovation achieved in these two fields has allowed for real-time observation of biological processes at the single-cell level simultaneously for large groups of neurons (Grienberger and Konnerth, 2012).

The output of two-photon calcium imaging is a movie of time-varying fluorescence intensities, and a first complex pre-processing phase deals with the identification of the spatial location of each neuron in the optical field and source extraction (Mukamel *et al.*, 2009; Dombek *et al.*, 2010). The resulting processed data consist of a fluorescent calcium trace for each observable neuron in the targeted area which, however, is only a proxy of the underlying neuronal activity. Hence further analyses are needed to deconvolve the fluorescence trace to extract the spike train (i.e. the series of recorded firing times), and to try to explain how these firing events are linked with the experiment that generated that particular pattern of activity.

1.1.1. Deconvolution methods

There is currently a rich literature of methods addressing the issue of deconvolving the raw fluorescent trace to extract the spike train. A successful approach is to assume a biophysical model to relate the spiking activity to the calcium dynamics, and to the observed fluorescence. Vogelstein *et al.* (2010) proposed a simple but effective model that has later been adopted by several authors (Pnevmatikakis *et al.*, 2016; Friedrich and Paninski, 2016; Friedrich *et al.*, 2017; Jewell and Witten, 2018; Jewell *et al.*, 2019). The model considers the observed fluorescence as a linear (and noisy) function of the intracellular calcium concentration; the calcium dynamics is then modeled using an autoregressive process with jumps in correspondence of the neuron's firing events. Denoting with y_t the observed fluorescence trace of a neuron and with Ca_t the

underlying calcium concentration, for time $t = 1, \dots, T$, the model can be written as

$$\begin{aligned} y_t &= b + \text{Ca}_t + \epsilon_t, \quad \epsilon_t \sim \text{N}(0, \sigma^2), \\ \text{Ca}_t &= \gamma \text{Ca}_{t-1} + A_t + w_t, \quad w_t \sim \text{N}(0, \tau^2), \end{aligned} \tag{1.1}$$

where b models the baseline level of the observed trace and ϵ_t is a Gaussian measurement error. In the absence of neuronal activity, the true calcium concentration Ca_t is considered to be centered around zero. The parameter A_t captures the neuronal activity: in the absence of a spike ($A_t = 0$), the calcium level follows a AR(1) process controlled by the parameter γ ; when a spike occurs, the concentration increases instantaneously of a value $A_t > 0$. A challenge remains estimating the neuronal activity A_t in a precise and computationally efficient way.

Vogelstein *et al.* (2010) assumed that all spikes have a fixed amplitude, and interpreted the parameter A_t as the *number* of spikes at time t . Following this definition, they placed a Poisson prior distribution on A_t ; however, the maximum a posteriori estimation of the spike train using a Poisson distribution is computationally intractable. Hence they searched an approximate solution by replacing the Poisson distribution with an exponential distribution of the same mean. This leads to some loss of interpretation of the parameters A_t , as now they are no longer integer values but rather non-negative real numbers, but turns the problem into a convex optimization, which can be solved efficiently. Adopting this approach leads to solving a non-negative lasso problem for estimating the calcium concentration, where the L_1 penalty enforces sparsity of the neural activity. Efficient algorithms to obtain a solution of this problem have also been proposed by Pnevmatikakis *et al.* (2016), Friedrich and Paninski (2016), and Friedrich *et al.* (2017).

A different perspective is instead proposed by Jewell and Witten (2018) and Jewell *et al.* (2019): rather than interpreting A_t in model (1.1) as the number of spikes at the t -th timestep, they interpreted its sign as an indicator for whether or not *at least one* spike occurred, that is, $A_t = 0$ indicates no spikes at time t , and $A_t > 0$ indicates the occurrence of at least one spike. The model so formulated includes an indicator variable, which corresponds to using an L_0 penalization and which makes the optimization problem highly non-convex. In their work, Jewell and Witten (2018) and Jewell *et al.* (2019) developed fast algorithms to compute the spike trains under these assumptions. Jewell and Witten (2018) asserted that the solutions discussed by Vogelstein *et al.* (2010), Friedrich and Paninski (2016), and Friedrich *et al.* (2017) can actually be seen as convex relaxations of this optimization problem, to overcome the computational intractability of the L_0 penalization.

Finally, Pnevmatikakis *et al.* (2013) proposed a fully Bayesian approach. Although less computationally efficient than optimization methods, it allows to obtain a posterior distribution of all model parameters instead of just a point estimate, hence improving uncertainty quantification. Differently from previous models, they defined the parameter A_t as the *amplitude* of a spike at time t , taking values in the non-negative real numbers. They formulated the presence/absence of a spike and its amplitude by using the product of a Bernoulli random variable (taking value 0 if there is no spike at time t , and 1 otherwise) with a half-Gaussian random variable (modeling the positive amplitudes). However, they did not explicitly assume sparsity of the spikes.

1.1.2. Spike train data analysis

Standard methods to analyze calcium imaging data rely on a two-step approach: in a first phase, some deconvolution method such as those just described is applied to identify the spikes, then, a different method is used on the deconvolved output to analyze it and, possibly, to relate it with some covariates. However, while there is a rich literature on deconvolution methods, there is still little research on methods that try to derive inferential results from their output.

Concerning encoding models, i.e. models that try to understand how the brain encodes external variables into spike train, Paninski *et al.* (2007) focused on the use of generalized linear models (GLMs). GLMs allow spike trains to be regressed against a potentially large number of covariates such as behavioral parameters, experimental conditions and other relevant factors. Moreover, regression models provide simple and interpretable results of the effect of each covariate on the neuronal response. In particular, Paninski *et al.* (2007) highlighted the importance of regularization methods and inclusion of prior knowledge to improve estimation of the model parameters, as in many cases the number of covariates is potentially very large, leading to noisy results and a loss in interpretability.

A different approach has been proposed by Wei *et al.* (2019): instead of focusing the relationship between the experimental conditions and some summary statistic of the resulting spike train, they studied the distribution of the deconvolved output. In particular, this allows to analyze quantities such as the spike probability and the spikes' amplitudes. They proposed a mixture model, with a Dirac mass at zero, representing the absence of neuronal response, and a translated Gamma distribution to model the positive amplitudes.

1.2. DATA SETS

Una frase introduttiva? Parlo dei dati dell'Allen Brain Observatory e poi ci sarebbe da mettere i nuovi dati se riesco a fare qualcosa del progetto 3...

1.2.1. Allen Brain Observatory data

The Allen Brain Observatory (Allen Institute for Brain Science, 2016) is a large public data repository for investigating how sensory stimulation is represented by neural activity in the mouse visual cortex in both single cells and populations. The project aims to provide a standardized and systematic survey to measure and analyze visual responses from neurons across cortical areas and layers, utilizing transgenic Cre lines to drive expression of genetically encoded fluorescent calcium indicators, and measured by *in vivo* two-photon calcium imaging.

The study is an extended survey of physiological activity in the mouse visual cortex in response to a range of visual stimuli (Allen Brain Observatory, 2017). Each mouse was placed in front of a screen where different types of visual stimuli were shown, while the mouse's neuronal activity was recorded. The stimuli vary from simple synthetic images such as locally sparse noise or static gratings, to complex natural scenes and movies. The goal of the study is to investigate how neurons at different depths and in different

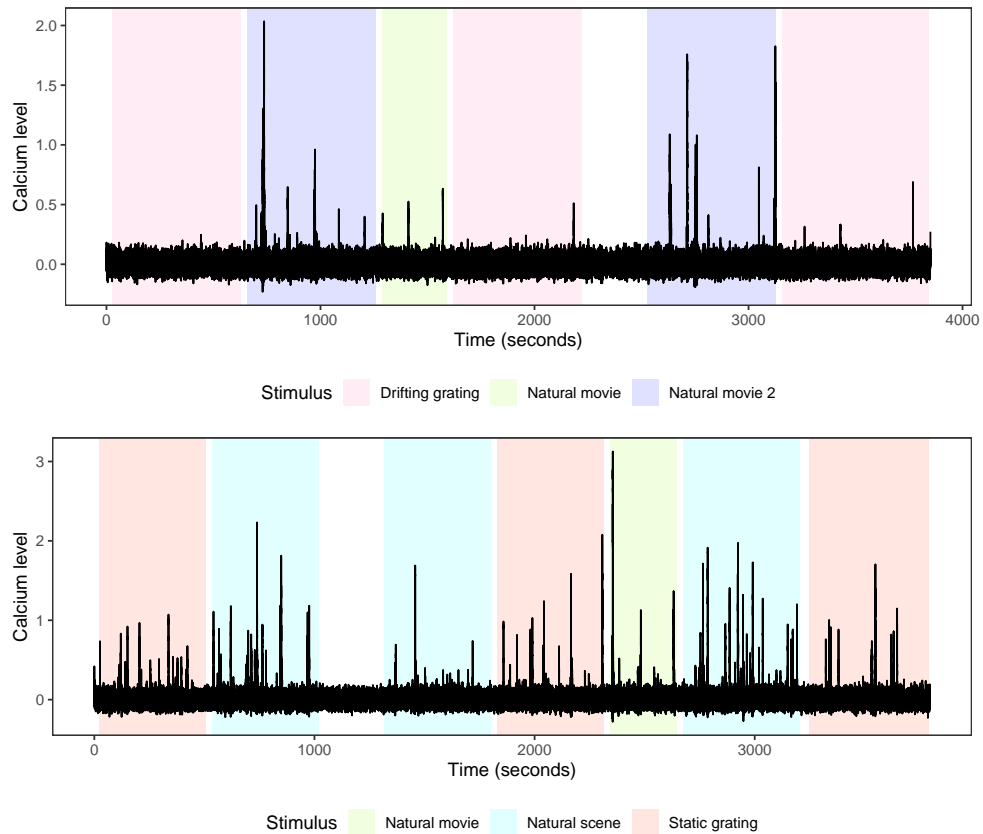


FIGURE 1.1: Allen Brain Observatory data: calcium traces (black line) of two neurons located in the primary visual area during Session A (upper plot) and Session B (bottom plot) of the experiment. The background colors denote the visual stimulus displayed at each time.

areas of the visual cortex respond to stimuli of varying complexity, to understand their functional properties. Specifically, each neuron in the visual cortex can be characterized by their *receptive field*, i.e. the features of the visual stimulus that trigger the signaling of that neuron. An important finding from mammalian is that higher visual areas tend to respond to more complex stimuli relative to lower areas. These differences indicate that the different neurons and visual areas have distinct functional properties. Hence, it is of critical interest to devise methods that allow inferring how the neuronal response varies under the different types of visual stimuli. As an example, Figure 1.1 shows the calcium traces of two neurons recorded during two different experiment sessions from the Allen Brain Observatory study. Each experiment comprises three types of visual stimuli, and has a duration of approximately one hour. These plots highlight that the neuronal response is highly variable, both across experimental conditions and between neurons.

The Allen Brain Observatory study comprises records of neuronal activity from over 60000 cells from six visual areas (VISp, VISl, VISal, VISrl, VISam, and VISpm) and different imaging depths (ranging from 175 to 625 microns). The data were collected analyzing the brain activity of several genetically engineered mice, using different transgenic Cre lines. The neuronal response of each mouse was recorded during three

experimental sessions: specifically, each session was made up of different types of visual stimuli displayed sequentially. Session “A” comprises two natural movies and a drifting gratings stimulus; session “B” comprises both natural movies and natural scenes, and a static gratings stimulus; finally, session “C” again includes two natural movies, and a locally sparse noise. Moreover, in all sessions a period of absence of stimuli was used to evaluate the baseline response during spontaneous activity. The synthetic stimuli are used to investigate the parameters that trigger the neuronal response: the locally sparse noise displays white and black spots in different parts of the visual space, and allows to map the spatial size and shape of the receptive field. The grating stimulus is a simple pattern whose intensity varies periodically along one dimension, and is constant in the other dimension. Different spatial frequencies, temporal frequencies and orientations are considered in order to further characterize the receptive fields. A detailed description of the visual stimuli can be found in a technical report (Allen Brain Observatory, 2017).

1.2.2. Altri dati?

Paragrafo qui.

1.3. A BRIEF REVIEW OF SOME BAYESIAN NONPARAMETRIC MODELS

In this section we review some statistical tools that will be employed in this thesis in the analysis of calcium imaging data. The purpose of this section is not to provide a comprehensive review, but rather to outline the theoretical framework we adopted and fix some notation. The core topic will be the Bayesian methodology, with a focus on Bayesian nonparametric models.

1.3.1. Finite mixture models

We start our discussion by reviewing finite mixtures. Although they are not part of the Bayesian nonparametric methodology, they provide the starting point for many models that we will review in the following. The content of this brief overview on finite mixtures is largely based on the dedicated chapter in Gelman *et al.* (2013).

Definition and hierarchical representations

Mixtures are a popular tool to model heterogeneous data, characterized by the presence of subpopulations within the overall population. In many practical problems the data are collected under different conditions – unfortunately, it is not always possible to have information on the subpopulation to which each individual observation belongs. Mixture models can be used in problems of this type, where the population consists of a number of latent subpopulations, and within each of them a relatively simple model can be applied.

Denote the observed data as a vector of n units $\mathbf{y} = (y_1, \dots, y_n)$; also, assume that the n observations are exchangeable, meaning that the joint probability density $p(y_1, \dots, y_n)$ is invariant to permutations of the indices. In the framework of finite

mixtures, we assume that the population is made of $K \leq n$ subpopulations, with K known and fixed. We assume that within each of these groups, the distribution of y_i , $i = 1, \dots, n$, can be modeled as $f(y_i | \theta_k^*)$, for $k = 1, \dots, K$. Usually a common parametric family is assumed for all these component distributions, which however depend on specific parameter vectors θ_k^* . The last missing piece to construct a mixture model is the parameter describing the proportion of population from each component k : we denote this parameter with π_k , satisfying $\sum_{k=1}^K \pi_k = 1$. Denoting the full vectors of parameters as $\boldsymbol{\theta}^* = (\theta_1^*, \dots, \theta_K^*)$ and $\boldsymbol{\pi} = (\pi_1, \dots, \pi_K)$, the data distribution for observation i can be formulated as

$$p(y_i | \boldsymbol{\theta}^*, \boldsymbol{\pi}) = \pi_1 f(y_i | \theta_1^*) + \dots + \pi_K f(y_i | \theta_K^*).$$

In mixture models it is convenient to think of the component indicators as missing data, and to impute them to obtain a much simpler form of the data distribution. Hence we introduce the indicator S_{ik} of component k for observation i , with

$$S_{ik} = \begin{cases} 1 & \text{if } y_i \text{ is drawn from component } k \\ 0 & \text{otherwise.} \end{cases}$$

Given $\boldsymbol{\pi}$, the distribution of $\mathbf{S}_i = (S_{i1}, \dots, S_{iK})$ is Multinomial($1; \pi_1, \dots, \pi_K$). Conditionally on \mathbf{S}_i , the data distribution of y_i is simply $p(y_i | \mathbf{S}_i, \boldsymbol{\theta}^*) = \prod_{k=1}^K f(y_i | \theta_k^*)^{S_{ik}}$; moreover, given $\mathbf{S} = (\mathbf{S}_1, \dots, \mathbf{S}_n)$, the y_i are assumed to be independent. The joint density of the observed data and the unobserved indicators, conditionally on the model parameters, can now be written as

$$p(\mathbf{y}, \mathbf{S} | \boldsymbol{\theta}^*, \boldsymbol{\pi}) = p(\mathbf{y} | \mathbf{S}, \boldsymbol{\theta}^*) p(\mathbf{S} | \boldsymbol{\pi}) = \prod_{i=1}^n \prod_{k=1}^K \{\pi_k f(y_i | \theta_k^*)\}^{S_{ik}}.$$

Having defined the data distribution, we need to specify adequate prior distributions on the model parameters $\boldsymbol{\pi}$ and $\boldsymbol{\theta}^*$. The prior G_0 on $\boldsymbol{\theta}^*$ is usually chosen depending on the specific application and on the basis of the component distribution f . For the mixture proportions π_k , the conjugate and most natural prior distribution is the Dirichlet distribution, $\boldsymbol{\pi} \sim \text{Dirichlet}_K(\alpha_1, \dots, \alpha_K)$.

This model also admits a useful hierarchical representation. Rewriting the latent allocation variables using the cluster indicators $c_i \in \{1, \dots, K\}$, with $c_i = k$ if y_i belongs to the k -th mixture component (i.e. $S_{ik} = 1$), the model is, for $i = 1, \dots, n$

$$\begin{aligned} y_i | c_i = k, \theta_k^* &\sim f(y_i | \theta_k^*) \\ \Pr(c_i = k | \pi_1, \dots, \pi_K) &= \pi_k \quad \text{for } k = 1, \dots, K \\ \theta_1^*, \dots, \theta_K^* &\sim G_0 \\ \pi_1, \dots, \pi_K &\sim \text{Dirichlet}_K(\alpha_1, \dots, \alpha_K). \end{aligned} \tag{1.2}$$

It is possible to rewrite Equation (1.2) in a slightly different way by thinking that each observation y_i is associated with a parameter θ_i , where these parameters are drawn from a discrete distribution G with support on the K locations $\{\theta_1^*, \dots, \theta_K^*\}$.

The model then becomes, for $i = 1, \dots, n$

$$\begin{aligned} y_i \mid \theta_i &\sim f(y_i \mid \theta_i) \\ \theta_i \mid \boldsymbol{\theta}^*, \boldsymbol{\pi} &\sim G = \sum_{k=1}^K \pi_k \delta_{\theta_k^*} \\ \theta_1^*, \dots, \theta_K^* &\sim G_0 \\ \pi_1, \dots, \pi_K &\sim \text{Dirichlet}_K(\alpha_1, \dots, \alpha_K). \end{aligned} \tag{1.3}$$

Posterior inference for finite mixture models

Posterior inference for mixture models is usually performed through Markov Chain Monte Carlo (MCMC) methods and, in particular, the Gibbs sampler, as the full conditionals after imputing the cluster indicators $\mathcal{C} = \{c_1, \dots, c_n\}$ are greatly simplified. Moreover, for the distribution of the mixture weights it is possible to exploit the conjugacy of the Dirichlet distribution with the multinomial model. A Gibbs sampler then simply iterates these three steps:

1. Update the cluster-specific parameters θ_k^* , for $k = 1, \dots, K$, from

$$p(\theta_k^* \mid \mathcal{C}, \mathbf{y}) \propto G_0(\theta_k^*) \prod_{i:c_i=k} f(y_i \mid \theta_k^*).$$

2. Update the weights π_1, \dots, π_K by sampling from a Dirichlet distribution with updated parameters

$$\pi_1, \dots, \pi_K \mid \mathcal{C} \sim \text{Dirichlet}_K(\alpha_1 + n_1, \dots, \alpha_K + n_K)$$

where n_k is the number of observations allocated to cluster k , for $k = 1, \dots, K$.

3. Update the cluster indicators: for $i = 1, \dots, n$ and $k = 1, \dots, K$,

$$\Pr(c_i = k \mid \boldsymbol{\pi}, \boldsymbol{\theta}^*, y_i) \propto \pi_k f(y_i \mid \theta_k^*).$$

1.3.2. Dirichlet process mixture models

Nonparametric mixtures extend model (1.3) by placing a nonparametric prior on G . The most common prior on random probability measures is the Dirichlet process (DP), introduced by Ferguson (1973, 1974). Draws from a DP are discrete distributions with probability one, hence they turned out useful as flexible mixing measures in discrete mixtures.

The Dirichlet process

The Dirichlet process is a stochastic process whose realizations are probability distributions with probability one. Stochastic processes are distributions over function spaces, with their realizations being random functions. In the case of the DP, it is a distribution over the space of probability measures, which are real-valued functions with particular

properties, which can be interpreted as distributions over some probability space. For this short review of some of the main properties of the DP we followed the unpublished report by Yee Whye Teh, which illustrates in a clear and simple way the fundamental properties of this process.

Formally, a random distribution G on some probability space Θ is said to follow a DP prior with base measure G_0 and concentration parameter α , denoted $G \sim \text{DP}(\alpha, G_0)$, if for any partition $\{B_1, \dots, B_H\}$ of Θ

$$(G(B_1), \dots, G(B_H)) \sim \text{Dirichlet}_H(\alpha G_0(B_1), \dots, \alpha G_0(B_H)).$$

That is, the finite-dimensional marginal distributions of a DP are Dirichlet distributions.

The success of the DP mainly arises from two appealing characteristics: its large support, with respect to the space of probability distributions, and tractability of the posterior distribution. Closely related to this last aspect is the conjugacy property of the DP: as the finite dimensional Dirichlet distribution is conjugate to the multinomial likelihood, the DP is conjugate with respect to i.i.d. sampling, that is, with respect to a completely unknown distribution from i.i.d. data. More precisely, if we take $\{\theta_1, \dots, \theta_n\}$ a sequence of independent draws from $G \sim \text{DP}(\alpha, G_0)$, then the posterior distribution of G given these observed values is still a DP. Letting again $\{B_1, \dots, B_H\}$ be a finite measurable partition of Θ , and letting n_h be the number of observed values in B_h , for $h = 1, \dots, H$, the posterior distribution is given by

$$(G(B_1), \dots, G(B_H)) \mid \theta_1, \dots, \theta_n \sim \text{Dirichlet}_H(\alpha G_0(B_1) + n_1, \dots, \alpha G_0(B_H) + n_H).$$

In other terms, the posterior distribution is still DP with updated parameters:

$$G \mid \theta_1, \dots, \theta_n \sim \text{DP}\left(\alpha + n, \frac{\alpha G_0 + \sum_{i=1}^n \delta_{\theta_i}}{\alpha + n}\right)$$

where the posterior base measure is a weighted average between the prior base measure G_0 and the empirical distribution $\sum_{i=1}^n \delta_{\theta_i}/n$. The weight associated with the prior base distribution is proportional to α , while the empirical distribution has weight proportional to the number of observations.

Another useful result, which allows to get a better understanding of the effect of using a DP as mixing measure, is the represented by Blackwell-MacQueen urn scheme (Blackwell and MacQueen, 1973), which describes the predictive distribution of draws from a DP. Consider again a sequence $\{\theta_1, \dots, \theta_n\}$ of independent draws from $G \sim \text{DP}(\alpha, G_0)$. The predictive distribution of θ_{n+1} conditioned on these values, and with G marginalized out is given by

$$\theta_{n+1} \mid \theta_1, \dots, \theta_n \sim \frac{1}{\alpha + n} \left(\alpha G_0 + \sum_{i=1}^n \delta_{\theta_i} \right).$$

Therefore the posterior base measure given $\{\theta_1, \dots, \theta_n\}$ is also the predictive distribution of θ_{n+1} . This distribution highlights the discreteness of draws from a DP, and allows to investigate the clustering structure induced by the DP when is used as mixing measure in mixture models. Since the distribution is discrete, it is possible that some of the values $\{\theta_1, \dots, \theta_n\}$ will be repeated. In particular, the unique values of $\{\theta_1, \dots, \theta_n\}$

induce a partition of the set $\{1, \dots, n\}$ into clusters defined by observations with the same value. Denoting with $\{\theta_1^*, \dots, \theta_K^*\}$ the unique values among the θ_i , and letting n_k be the number of θ_i equal to θ_k^* , for $i = 1, \dots, n$ and $k = 1, \dots, K$, the predictive distribution can be written as

$$\theta_{n+1} \mid \theta_1, \dots, \theta_n \sim \frac{1}{\alpha + n} \left(\alpha G_0 + \sum_{k=1}^K n_k \delta_{\theta_k^*} \right).$$

From this equation, it is possible to notice that θ_{n+1} will take a value θ_k^* with a probability proportional to n_k , the number of times it has already been observed. Hence, the larger n_k is, the higher the probability that it will grow. This is a rich-gets-richer phenomenon, where large clusters grow larger faster.

The DP admits several nice representations. An intuitive constructive definition of a DP random probability measure is given by Sethuraman (1994) and is based on the discrete nature of the process, which can be represented as a weighted sum of point masses. This definition states that if $G \sim \text{DP}(\alpha, G_0)$, then it can be expressed as follows:

$$\begin{aligned} v_k &\sim \text{Beta}(1, \alpha), \quad \theta_k^* \sim G_0 \quad \text{for } k \geq 1 \\ \pi_1 &= v_1, \quad \pi_k = v_k \prod_{h=1}^{k-1} (1 - v_h) \quad \text{for } k \geq 2 \\ G &= \sum_{k=1}^{\infty} \pi_k \delta_{\theta_k^*}. \end{aligned} \tag{1.4}$$

The construction of the weights $\{\pi_k\}_{k=1}^{\infty}$ by means of beta random variable is usually called stick-breaking process, also denoted as $\pi \sim \text{GEM}(\alpha)$ after the names of Griffiths, Engen and McCloskey. The name arises from a metaphor for this construction, where a unit stick is broken in infinitely many parts, and each piece is used to define a weight. Because of its simplicity, this representation has motivated extensions of the process as well as new inference procedures, as for example the algorithms described in the following to sample from the posterior distribution of Dirichlet process mixtures.

Dirichlet process mixtures

Getting back to the framework of mixture models, from the representation of the process as discrete measure it is straightforward to extend the finite mixtures described in the previous section to nonparametric mixtures: following the structure of Equation (1.3), DP mixtures (DPMs) can be written as

$$\begin{aligned} y_i \mid \theta_i &\sim f(y_i \mid \theta_i) \\ \theta_i \mid G &\sim G \\ G &\sim \text{DP}(\alpha, G_0). \end{aligned}$$

Alternatively, making use of the set of unique values $\{\theta_k^*\}_{k=1}^{\infty}$ and of Sethuraman's representation, the model can be expressed as

$$p(y_i \mid G) = \sum_{k=1}^{\infty} \pi_k f(y_i \mid \theta_k^*) \tag{1.5}$$

where the weights $\{\pi_k\}_{k=1}^{\infty}$ follow a stick-breaking construction and the $\{\theta_k^*\}_{k=1}^{\infty}$ are i.i.d. samples from the base measure G_0 .

Differently from finite mixtures, DPMs are infinite mixture models, as they assume a countably infinite number of components. However, because the π_k 's decrease exponentially quickly, only a small number of components will be used to model the data a priori: in the following, we will define *clusters* these non-empty components. In general, the prior expected number of clusters in a sample of size n is approximately equal to $\alpha \log(1 + n/\alpha)$. This means that while in finite mixture models the number of clusters has to be fixed in advance, in DPMs the number of clusters is determined by the data and can be inferred.

Posterior inference for DPMs

Applying MCMC techniques to DPMs directly is not feasible, as it would require imputing the infinite-dimensional distribution G . Instead, successful algorithms to perform posterior inference on DP mixtures have been developed using the particular representations that this process admits. It is common to divide these methods into two classes depending on the strategy they adopt to deal with the infinite-dimensional component of the model: marginal algorithms are based on model representations with the DP is integrated out, while conditional algorithms explicitly represent the measure generated by the process using its stick-breaking construction. Here we will focus on conditional methods. Avoiding marginalization of the random measure allows to perform inference on it directly, moreover, these methods are often computationally more efficient than marginal ones; however, they require to devise good strategies to deal with the infinite dimension of the process.

In the blocked Gibbs sampler of Ishwaran and James (2001) the infinite random measure is truncated to an upper bound K for the number of clusters. The motivation that justifies this approach is that the weights $\{\pi_k\}_{k=1}^{\infty}$ determined by the stick-breaking construction are stochastically decreasing in k . By choosing a sufficiently large value K one can assume that $\sum_{k=K+1}^{\infty} \pi_k$ has a distribution concentrated near zero. Adopting such truncation leads to a representation of the model as finite mixture, so the sampler described in Section 1.3.1 can be applied with just few changes on the weights distribution. In particular, the weights are now sampled from a stick-breaking process with $v_k \sim \text{Beta}(1 + n_k, \alpha + \sum_{h=k+1}^K n_h)$ for $k = 1, \dots, K - 1$. Finally, letting $v_K = 1$ ensures that the first K weights sum to one. Adopting this approach leads to a straightforward MCMC algorithm for posterior inference, however, in some applications K needs to be set to very large values in order to obtain an adequate approximation.

The slice sampler (Walker, 2007; Kalli *et al.*, 2011) has been adopted as an alternative “dynamic” truncation method to automatically select the active components of the mixture. The slice sampler relies on the introduction of latent uniform random variables u_i , $i = 1, \dots, n$, such that marginalizing the joint density of (y_i, u_i) still returns the desired density in Eq. (1.5), and such that the conditional density of $y_i \mid u_i$ only involves a finite number of mixture components. Specifically, model (1.5) can be obtained as marginal density with respect to u_i of

$$p(y_i, u_i \mid G) = \sum_{k=1}^{\infty} \mathbb{I}(u_i < \pi_k) f(y_i \mid \theta_k^*),$$

where $\mathbb{I}(A)$ is the indicator variable, taking value 1 if event A occurs and 0 otherwise. The key of introducing this variable is that, conditionally on u_i , the density can be written as

$$p(y_i | u_i, G) = N_u^{-1} \sum_{k \in A_u} f(y_i | \theta_k^*)$$

where A_u is the set of indices of active components $A_u = \{k : \pi_k > u\}$ and $N_u = \sum_{k \in A_u} \pi_k$. This model defines a finite mixture with equal weights N_u^{-1} . Introducing the cluster indicators $\mathcal{C} = \{c_1, \dots, c_n\}$ further simplifies the density, similarly to the case of finite mixtures. Finally, Kalli *et al.* (2011) also introduce a non-stochastic positive sequence $\{\xi_1, \xi_2, \dots\}$ in order to improve mixing (we refer to the original paper for a discussion on the choice of the sequence). With all these elements, the joint density of $(\mathbf{y}, \mathbf{u}, \mathcal{C})$ conditioned on $\boldsymbol{\pi}$ and $\boldsymbol{\theta}^*$ becomes

$$p(\mathbf{y}, \mathbf{u}, \mathcal{C} | \boldsymbol{\pi}, \boldsymbol{\theta}^*) = \prod_{i=1}^n \mathbb{I}(u_i < \xi_{c_i}) \frac{\pi_{c_i}}{\xi_{c_i}} f(y_i | \theta_{c_i}^*). \quad (1.6)$$

The slice sampler algorithm iterates the following steps:

1. Update the cluster-specific parameters θ_k^* , for $k = 1, \dots, K$, where K is defined as the maximum index h such that $\xi_h > u_i$ for all $i = 1, \dots, n$, from

$$p(\theta^* | \mathcal{C}) \propto G_0(\theta_k^*) \prod_{i:c_i=k} f(y_i | \theta_k^*).$$

2. Update the weights π_k for $k = 1, \dots, K$ using the stick-breaking construction (1.4) with beta random variables $v_k \sim \text{Beta}(1 + n_k, \alpha + \sum_{h=k+1}^K n_h)$.
3. Sample the latent variables u_i from a uniform distribution $u_i | c_i \sim \text{Unif}(0, \xi_{c_i})$
4. Update the cluster allocations c_i for $i = 1, \dots, n$ from

$$\Pr(c_i = k | u_i, y_i, \theta_k^*) \propto \mathbb{I}(k : \xi_k > u_i) \frac{\pi_k}{\xi_k} f(y_i | \theta_k^*).$$

1.3.3. Mixtures of finite mixtures

To avoid fixing the number of clusters, a different approach to DP mixtures is to consider finite mixtures with a prior on the number of components. Although this may seem as the most natural way to infer the number of groups, application of mixtures of finite mixtures (MFMs) has long been hindered by the difficulty of performing posterior inference. Several inference methods have been proposed for this type of models (McCullagh and Yang, 2008; Nobile, 2004; Nobile and Fearnside, 2007; Richardson and Green, 1997) often exploiting the reversible jump Markov chain Monte Carlo techniques. However, applying the reversible jump in new situations can be hard, as it requires designing new reversible jump moves.

More recently, different models have been proposed inspired by nonparametric mixtures. Miller and Harrison (2018) explicitly derived MFMs counterparts for several properties exhibited by DPMs. They considered a finite mixture model similar to the

one defined in section 1.3.1, where however the number of clusters is random and is assigned a prior distribution. A main limitation of their approach is that it assumes a fixed parameter α for the Dirichlet distribution, regardless of the dimension K , which can lead to undesired

Another approach is discussed by Malsiner-Walli *et al.* (2016) and Frühwirth-Schnatter and Malsiner-Walli (2019), based on the use of sparse mixtures. Similarly to DPMs, in this formulation they distinguish between the mixture components and the clusters, which are defined as the components actually used by the data. In their approach, the number of components K is fixed to a large and clearly overfitting value, and a Dirichlet prior with small parameter on the mixture weights ensures that the (random) number of clusters K_+ will take values smaller than K with high probability a priori and also a posteriori.

Generalized mixtures of finite mixtures

A general formulation that includes all three models described above as special cases (finite mixtures with a fixed number of clusters, MFMs and overfitted mixtures) has recently been described by Frühwirth-Schnatter *et al.* (2020): they call this specification generalized mixture of finite mixtures (gMFM). Similarly to overfitted mixtures, a key aspect of this approach is the distinction between the number of components K and the number of clusters K_+ ; however, here, the number of components is also random. In the following we will review some aspects of these models that will be used later in this thesis. The gMFM model can be defined in a hierarchical form analogous to Equation (1.2) as

$$\begin{aligned} y_i | K, c_i = k, \theta_k^* &\sim f(y_i | \theta_k^*) \\ \Pr(c_i = k | K, \pi_1, \dots, \pi_K) &= \pi_k \quad \text{for } k = 1, \dots, K \\ \theta_1^*, \dots, \theta_K^* &\sim G_0 \\ \pi_1, \dots, \pi_K | K, \alpha &\sim \text{Dirichlet}_K(\alpha/K, \dots, \alpha/K) \\ K &\sim p(K) \end{aligned}$$

Including a prior on K also induces a prior on the number of clusters K_+ : here a crucial role is played by the sequence of concentration parameters of the Dirichlet distribution. Considering fixed parameters as in Miller and Harrison (2018), where a $\text{Dirichlet}_K(1, \dots, 1)$ is used regardless of the value of K , leads to a prior expected number of clusters $E(K_+)$ close to $E(K)$ for many priors $p(K)$. Having instead concentration parameters that decrease with increasing K induces randomness in the prior distribution of $K_+ | K$, allowing for a gap between K_+ and K . In this formulation the parameters decrease linearly with K , and a F prior distribution is used for the hyperparameter α . The specification of a gMFM is completed with a suitable prior $p(K)$ on the number of components. In their work, Frühwirth-Schnatter *et al.* (2020) discuss different choices and compare the resulting prior on the number of clusters. A desirable prior on K should be weakly informative on the number of clusters, and should lead to a prior on K_+ which is concentrated on moderate number of clusters, with fat tails to ensure that also a high number of clusters may be estimated. They suggest to use a translated prior for K , where $K - 1$ follows a beta-negative-binomial

distribution, which is a hierarchical generalization of the Poisson, the geometric and the negative-binomial distribution.

Posterior inference for gMFMs

An important contribution of the work of Frühwirth-Schnatter *et al.* (2020) is the introduction of a new inference algorithm “telescoping sampler” to obtain the posterior distribution of all model parameters without resorting to reversible jump MCMC techniques. Their algorithm is a trans-dimensional Gibbs sampler which at each iteration alternates two key steps: first, it updates the partition of the observations $\mathcal{C} = \{c_1, \dots, c_n\}$ conditionally on the number of components, then, it samples a new value for K on the basis of this partition. Explicitly sampling the number of mixture components greatly simplifies inference as, conditionally on K , the updates of the partition and of the model parameters are brought back to standard steps. Hence the crucial aspect is sampling from the full conditional of the number of components. This is achieved by combining the conditional exchangeable partition probability function $p(\mathcal{C} \mid n, K, \alpha)$, derived in Section 2.2 of Frühwirth-Schnatter *et al.* (2020), with the prior $p(K)$. The algorithm performs the following steps:

1. Update the partition \mathcal{C} :
 - (a) Sample c_i , for $i = 1, \dots, n$ from $\Pr(c_i = k \mid \boldsymbol{\pi}, \boldsymbol{\theta}^*, y) \propto \pi_k f(y_i \mid \theta_k^*)$;
 - (b) Determine the number K_+ of non-empty clusters and relabel the components such that the first K_+ clusters are non-empty.
2. Conditional on \mathcal{C} , update the parameters of the non-empty components (and eventual hyperparameters):

$$p(\theta_k^* \mid \mathcal{C}, \mathbf{y}) \propto G_0(\boldsymbol{\theta}^*) \prod_{i:c_i=k} f(y_i \mid \theta_k^*) \quad \text{for } k = 1, \dots, K.$$

3. Conditional on \mathcal{C} , draw a new value for K from

$$p(K \mid \mathcal{C}, \alpha) \propto p(\mathcal{C} \mid n, K, \alpha) p(K) = p(K) \frac{K! \alpha^{K_+}}{(K - K_+)! K^{K_+}} \prod_{k=1}^{K_+} \frac{\Gamma(n_k + \alpha/K)}{\Gamma(1 + \alpha/K)}$$

for $K = K_+, K_+ + 1, \dots$; where n_k is the number of observations in cluster k .

4. Update α by performing a Metropolis-Hastings step to sample α from its full conditional

$$p(\alpha \mid \mathcal{C}, K) \propto p(\alpha) \frac{\alpha^{K_+ \Gamma(\alpha)}}{\Gamma(n + \alpha)} \prod_{k=1}^{K_+} \frac{\Gamma(n_k + \alpha/K)}{\Gamma(1 + \alpha/K)}$$

5. Add $K - K_+$ empty components,
 - (a) if $K > K_+$, sample $K - K_+$ new values θ_k^* from the prior, $k = K_+ + 1, \dots, K$;
 - (b) update the weight vector as

$$\pi_1, \dots, \pi_K \mid K, \alpha, \mathcal{C} \sim \text{Dirichlet}_K(\alpha/K + n_1, \dots, \alpha/K + n_K).$$

1.3.4. Bayesian nonparametric models for nested data

All models described so far assumed that the data were exchangeable, that is, they arise from one unknown distribution. However, there is growing interest in modeling scenarios where the data come from different but related groups, as for example different populations or experiments. In these cases it is desirable to individually model the distribution of each group, while also borrowing information between them. When data are collected from individuals in multiple groups, the exchangeability assumption is no longer valid: in these cases, observations are said to be partially exchangeable, meaning that they are exchangeable *within* groups.

Suppose that in addition to each $y_i, i = 1, \dots, n$, we also observe a categorical variable g_i with values in $\{1, \dots, J\}$ indicating the population to which y_i belongs, so that when $g_i = j$ means that y_i comes from the j -th group. In the Bayesian nonparametric framework, several approaches have been proposed to deal with these nested data sets.

The hierarchical Dirichlet process (Teh *et al.*, 2006) arises from the desire to flexibly model the distributions of the observations of each group, while also performing clustering to capture latent structures among all individuals. Each group-specific distribution is modeled with a mixture model which uses a random probability measure G_j as mixing measure, where the G_j 's are distributed according to a DP: this allows to obtain a partition of individuals within each group. In order to borrow information across groups, they propose a hierarchical formulation where one draw from a Dirichlet process is used as the base measure G_0 of the Dirichlet process generating the individual G_j 's. This construction implies that the distributions $\{G_1, \dots, G_J\}$ share the same atoms (the atoms of G_0), thus the model yields a clustering of the individuals also across groups. However, as these G_j 's are independent draws, in general, they will have different weights: as a result, there is no clustering of these group-specific distributions. The hierarchical DP hence does not allow to investigate similarities between the distributions, but only to cluster individuals.

To overcome this limitation, Rodríguez *et al.* (2008) introduced the nested Dirichlet process, which allows to obtain a clustering both of the observations within each group, and of the groups themselves. Consider again a collection of distributions $\{G_1, \dots, G_J\}$ serving as group-specific mixing measures of a nonparametric mixture. The nested DP assumes that $G_j | Q \sim Q$ for $j = 1, \dots, J$ and $Q \sim DP(\alpha, DP(\beta, G_0))$. Using the stick-breaking representation of the DP, this model can be expressed as

$$G_1, \dots, G_J | Q \sim Q, \quad Q = \sum_{k=1}^{\infty} \pi_k \delta_{G_k^*} \quad (1.7)$$

$$G_k^* = \sum_{l=1}^{\infty} \omega_{l,k} \delta_{\theta_{l,k}^*}$$

where the sequences of weights $\{\pi_k\}_{k=1}^{\infty}$ and $\{\omega_{l,k}\}_{l=1}^{\infty}$ for $k \geq 1$ follow a stick breaking construction, $\pi \sim \text{GEM}(\alpha)$ and $\omega_k \sim \text{GEM}(\beta)$, and the parameters $\theta_{l,k}^*$ are i.i.d. samples from G_0 . A main difference from the hierarchical DP is that this formulation allows to cluster the group-specific distributions: indeed, if two G_j 's are assigned to the same G_k^* , then the observations in the two groups have exactly the same generating distribution. When two groups share the same distribution, they are said to belong to the same distributional cluster.

In a recent paper by Camerlenghi *et al.* (2019), however, they noted a degeneracy property that occurs in the nested DP in case of ties across samples at the observed or latent level. In particular, if two distributions G_1 and G_2 share at least one atom, then their posterior distribution degenerates on $\{G_1 = G_2\}$, forcing homogeneity across the two samples. To overcome this drawback, they introduce a novel class of latent nested processes. These processes are based on a mixture of two random distributions: an idiosyncratic component and a shared component. The shared random distribution explicitly accounts for the possibility of observing some common atoms, while the idiosyncratic one allows some atoms to be distinct and specific to each subpopulation. However, implementation of this model becomes challenging and computationally burdensome when the number of groups increases.

The common atoms model

Another nested nonparametric prior, more suited to practical applications, is proposed by Denti *et al.* (2021). They formulate a constrained modification of the nested DP which, however, does not suffer from the degeneracy issue. Moreover, compared to the models introduced by Camerlenghi *et al.* (2019), it is computationally more efficient and allows to perform posterior inference in a quite straightforward way even when the number of groups is moderate. The first level of their common atoms model (CAM) is analogous to the nested DP (Eq. 1.7), however, the specification of the distributional atoms G_k^* makes use of a common set of atoms for all k . Hence the distributions G_k^* can be seen as realizations of a single-atom dependent DP,

$$G_k^* = \sum_{l=1}^{\infty} \omega_{l,k} \delta_{\theta_l^*}$$

where the sequences of weights $\{\omega_{l,k}\}_{l=1}^{\infty}$ for $k \geq 1$ again follow a stick breaking construction, and the common atoms $\{\theta_l^*\}_{l=1}^{\infty}$ are independent draws from a base measure G_0 . Similarly to the nested DP, the first mixture level of the CAM allows to perform a clustering of the group-specific distributions G_j ; however, as the set of atoms defining the G_k^* is common across distributions, the CAM also allows to obtain a clustering of individuals both within each group and across them, in a similar fashion to the hierarchical DP.

Convoluting this nested prior with a kernel we obtain a nested infinite mixture model: the density for observations $\mathbf{y}_j = \{y_i : g_i = j; i = 1, \dots, n\}$ belonging to group j can be written as

$$p(\mathbf{y}_j \mid \boldsymbol{\theta}^*, \boldsymbol{\pi}, \boldsymbol{\omega}) = \sum_{k=1}^{\infty} \pi_k \prod_{i: g_i=j} \sum_{l=1}^{\infty} \omega_{l,k} f(y_i \mid \theta_l^*).$$

Introducing two sequences of latent cluster allocations $\mathcal{C}^D = \{c_{g_i}^D\}$ and $\mathcal{C} = \{c_i\}$ for $i = 1, \dots, n$, corresponding respectively to the distributional cluster allocation of the J groups and to the observational cluster allocation of individuals, the model admits a

hierarchical representation as

$$\begin{aligned}
y_i &| c_i, \boldsymbol{\theta}^* \sim f(y_i | \boldsymbol{\theta}_{c_i}^*) \\
c_i | c_{g_i}^D = k, \boldsymbol{\omega}_k &\sim \sum_{l=1}^{\infty} \omega_{l,k} \delta_l \quad \boldsymbol{\omega}_k \sim \text{GEM}(\beta) \quad \text{for } k \geq 1 \\
c_{g_i}^D | \boldsymbol{\pi} &\sim \sum_{k=1}^{\infty} \pi_k \delta_k \quad \boldsymbol{\pi} \sim \text{GEM}(\alpha) \\
\theta_l^* &\sim G_0 \quad \text{for } l \geq 1.
\end{aligned}$$

Posterior inference for the CAM

To infer on the posterior distribution of the CAM model, Denti *et al.* (2021) develop a nested version of the slice sampler of Kalli *et al.* (2011) (described in the last part of Section 1.3.2). This sampler relies on two sequences of latent uniform variables $\mathbf{u}^D = \{u_{g_i}\}_{g_i=1}^J$ (on the distributional level) and $\mathbf{u}^O = \{u_i^O\}_{i=1}^n$ (on the observational level) pointing to the active mixture components. Moreover, they also introduce two deterministic sequences $\boldsymbol{\xi}^D = \{\xi_k\}_{k=1}^{\infty}$ and $\boldsymbol{\xi}^O = \{\xi_{l,k}^O\}_{l=1}^{\infty}$ for $k \geq 1$. Similarly to Equation 1.6, the model can be written as

$$p(\mathbf{y}, \mathbf{u}^D, \mathbf{u}^O, \mathcal{C}^D, \mathcal{C} | \boldsymbol{\theta}^*, \boldsymbol{\pi}, \boldsymbol{\omega}) = \prod_{j=1}^J \mathbb{I}(u_j^D < \xi_{c_j^D}^D) \frac{\pi_{c_j^D}}{\xi_{c_j^D}^D} \prod_{i:g_i=j} \mathbb{I}(u_i^O < \xi_{c_i, c_j^D}^O) \frac{\omega_{c_i, c_j^D}}{\xi_{c_i, c_j^D}^O} f(y_i | \boldsymbol{\theta}_{c_i}^*).$$

Then, the algorithm iterates the following steps

1. Sample the latent uniform random variables
 - (a) At the distributional level, for $j = 1, \dots, J$, sample $u_j^D \sim \text{Unif}(0, \xi_{c_j^D}^D)$
 - (b) At the observational level, for $i = 1, \dots, n$, sample $u_i^O \sim \text{Unif}(0, \xi_{c_i, c_{g_i}^D}^O)$
2. Update the weight vectors $\boldsymbol{\pi}$ and $\boldsymbol{\omega}_k$, for $k \geq 1$
 - (a) At the distributional level, sample the distributional stick-breaking proportions $v_k \sim \text{Beta}(1 + m_k, \alpha + \sum_{h=k+1}^{K^*} m_h)$, where m_k is the number of groups in distributional cluster k .
 - (b) At the observational level, for each $k = 1, \dots, K^*$, sample the stick-breaking proportions $u_{l,k} \sim \text{Beta}(1 + n_l^k, \beta + \sum_{h=l+1}^{L^*} n_h^k)$, where n_l^k is the number of individuals assigned to observational cluster l and distributional cluster k .
3. Update the cluster indicators
 - (a) For the distributional clusters, sample the variables c_j^D from

$$\Pr(c_j^D = k | \mathbf{u}^D, \boldsymbol{\pi}, \boldsymbol{\omega}_k, \mathcal{C}) \propto \mathbb{I}(u_j^D < \xi_{c_j^D}^D) \frac{\pi_{c_j^D}}{\xi_{c_j^D}^D} \prod_{i:g_i=j} \omega_{c_i, k}$$

(b) For the observational clusters, sample the variables c_i from

$$\Pr(c_i = l \mid y_i, g_i = j, c_j^D, \mathbf{u}^O, \omega_{l,c_j^D}) \propto \mathbb{I}(u_i^O < \xi_{l,c_j^D}^O) \frac{\omega_{l,c_j^D}}{\xi_{l,c_j^D}^O} f(y_i \mid \theta_l^*).$$

4. Conditional on the observational clusters, sample the cluster-specific parameters θ_l^* from

$$p(\theta^* \mid \mathcal{C}) \propto G_0(\theta_l^*) \prod_{i:c_i=l} f(y_i \mid \theta_l^*).$$

We refer to the Supplementary Material of the original paper for details about the specific sequences ξ^O and ξ^D and computation of the upper bounds K^* and L^* involved at step 2.

2 | EFFICIENT POSTERIOR SAMPLING FOR BAYESIAN POISSON REGRESSION

As we have seen in Section 1.1.2, encoding models are an important tool to study how the deconvolved spike trains vary with the underlying experimental conditions. To this end, GLMs provide a simple and flexible strategy to estimate the impact of each covariate on the mean of the variable of interest. A relevant question that can be addressed using GLMs is how the number of spikes detected during a specific experiment is affected by the experimental conditions and the characteristics of the neurons. A plausible assumption to model the spike counts per time bin is to use a Poisson distribution (Paninski *et al.*, 2007): in the context of GLMs, this setting naturally leads to the use of Poisson regression models.

Poisson regression models are common in statistics and represent one of the most popular choices to model how the distribution of count data varies with predictors. A typical assumption is that, under an independent sample of counts, y_1, \dots, y_n , the probability mass function of the generic y_i conditionally on a p -dimensional vector of covariates x_i is

$$f(y_i | \lambda_i) = \frac{\lambda_i^{y_i}}{y_i!} e^{-\lambda_i}, \quad \log(\lambda_i) = x_i^T \beta, \quad (2.1)$$

where β is a p -dimensional vector of unknown coefficients. Linking the linear predictor $x_i^T \beta$ and the parameter λ_i with the logarithm represents the most natural choice, as the logarithm is the canonical link for the Poisson family (Nelder and Wedderburn, 1972). Besides encoding models for spike train analyses, this model has broad application in several fields, including medicine and epidemiology (Frome, 1983; Frome and Checkoway, 1985; Hutchinson and Holtman, 2005), manufacturing process control (Lambert, 1992), analysis of accident rates (Joshua and Garber, 1990; Miaou, 1994), and crowd counting (Chan and Vasconcelos, 2009), among others.

Adopting a Bayesian approach can be particularly convenient in the context of calcium imaging studies. As pointed out by Paninski *et al.* (2007), often some regularization technique is needed to obtain reliable estimates of the effects, as in some experiments the large number of covariates leads to a sensible risk of overfitting. The Bayesian paradigm offers a natural approach to regularized regression: there is a large literature on prior inducing some kind of shrinkage or selection, as, for example, the spike-and-slab prior (Mitchell and Beauchamp, 1988), the Bayesian lasso (Park and Casella, 2008), the horseshoe prior and its extensions (Carvalho *et al.*, 2010; Piironen and Vehtari, 2017).

However, model (2.1) does not enjoy any conjugacy property and, thus, regardless of the prior used, the posterior distribution of β is not available in close form. Consequently, inference is conducted using Markov Chain Monte Carlo (MCMC) methods, which obtain a sample from the posterior distribution of the parameters.

Several approaches have focused on how to easily obtain the posterior distribution of the coefficients of Poisson models without requiring complex tuning strategies or long computation times. In the context of count-valued time series, Frühwirth-Schnatter and Wagner (2006) proposed a formulation of the model based on two levels of data augmentation, to derive an efficient approximate Gibbs sampler. Frühwirth-Schnatter *et al.* (2009) exploited a data augmentation strategy to simplify the computation of hierarchical models for count and multinomial data. Data augmentation strategies have also been employed in the case of models for multivariate dependent count data (Karlis and Meligkotsidou, 2005; Bradley *et al.*, 2018). However, the simplest Poisson regression in (2.1) still lacks a specific and efficient algorithm to sample from the posterior distribution of the parameters β for any prior choice, making the Metropolis-Hastings (Hastings, 1970) or Hamiltonian Monte Carlo (HMC) (Neal, 2011) algorithms the only available options.

On the other hand, several efficient computational strategies for binary regression models have been proposed in the literature. Using the probit link, Albert and Chib (1993) proposed an efficient data augmentation based on a latent Gaussian variable, while the more recent contribution by Polson *et al.* (2013) exploited the canonical logit link, introducing an efficient Pólya-gamma data augmentation scheme. Leveraging Polson *et al.* (2013) approach, we propose a novel approximation of the posterior distribution that can be exploited as proposal distribution of a Metropolis-Hastings algorithm or as importance density of an importance sampling for Poisson log-linear models with conditional Gaussian prior distributions on the regression parameters. With conditional Gaussian prior, we refer to a possibly hierarchical prior with conditional distribution $\beta \sim N(b, B)$, with b and/or B random. Examples include straightforward Gaussian prior distributions with informative (b, B) fixed using prior information, and scale mixtures of Gaussian where b is set to zero and the variance has a suitable hierarchical representation, such as the Bayesian lasso prior or the horseshoe prior, among others.

More specifically, we introduce an approximation of the posterior density that exploits the negative binomial convergence to the Poisson distribution. Thanks to this result, we are able to leverage the Pólya-gamma data augmentation scheme of Polson *et al.* (2013) to derive an efficient sampling scheme. In the next section, we introduce and discuss the proposed algorithms, starting from the definition of an *approximate* posterior distribution whose sampling can be performed straightforwardly. Sampling from this approximate posterior is then used as proposal density for the Metropolis-Hastings or importance sampler. The performance of the proposed algorithms in terms of computational efficiency is compared with that of state-of-the-art methods in a simulation study. Finally, we employ the proposed method to estimate a deconvolution model on spike train data from the Allen Brain Observatory.

2.1. EFFICIENT POSTERIOR SAMPLING STRATEGIES

2.1.1. Approximate posterior distribution

Assume y_1, \dots, y_n is an independent sample of counts from model (2.1). We introduce an approximation of the posterior density which exploits the negative binomial convergence to the Poisson distribution, i.e., we approximate the i -th contribution to the likelihood function $f(y_i | \lambda_i)$ with $\tilde{f}_{r_i}(y_i | \lambda_i)$ where

$$\tilde{f}_{r_i}(y_i | \lambda_i) = \left(\frac{r_i}{r_i + \lambda_i} \right)^{r_i} \left(\frac{\lambda_i}{r_i + \lambda_i} \right)^{y_i}, \quad (2.2)$$

which corresponds to the probability mass function of a negative binomial random variable with parameter r_i , the number of failures until the experiment is stopped, and success probability $\lambda_i/(r_i + \lambda_i)$. As r_i approaches infinity, this quantity converges to a Poisson likelihood.

Following Polson *et al.* (2013), we rewrite each i -th contribution to the approximate likelihood (2.2) by introducing augmented Pólya-gamma random variables $\omega_i \sim \text{PG}(y_i + r_i, 0)$, i.e

$$\begin{aligned} \tilde{f}_{r_i}(y_i | \beta) = \exp \left\{ \frac{(x_i^T \beta - \log r_i)(y_i - r_i)}{2} \right\} 2^{-(y_i + r_i)} \times \\ \int_0^{+\infty} \exp \left\{ -\omega_i \frac{(x_i^T \beta - \log r_i)^2}{2} \right\} f_{\text{PG}}(\omega_i; y_i + r_i, 0) d\omega_i, \end{aligned}$$

where $f_{\text{PG}}(\cdot; \xi, \zeta)$ denotes the density of a Pólya-gamma with parameters (ξ, ζ) .

In what follows, we assume that prior knowledge about the unknown β parameters is represented by a conditionally Gaussian prior, i.e. $\beta \sim \text{N}(b, B)$, with a possible hierarchical representation for the parameters b and B . Examples include default informative Gaussian with fixed (b, B) or scale mixtures of Gaussian where b is set to zero and the variance has a suitable hierarchical representation (Park and Casella, 2008; Carvalho *et al.*, 2010; Piiironen and Vehtari, 2017).

The *approximate* posterior based on the conditionally Gaussian prior $\beta \sim \text{N}(b, B)$ and approximate likelihood $\prod_{i=1}^n \tilde{f}_{r_i}(y_i | \beta)$ is consistent with the successful Gibbs sampler of Polson *et al.* (2013); i.e., sampling from the *approximate* posterior is equivalent to sampling iteratively from the following full conditionals

$$\omega_i | \beta \sim \text{PG}(y_i + r_i, x_i^T \beta - \log r_i), \quad \beta | y, \omega \sim \text{N}_p(m_\omega, V_\omega), \quad (2.3)$$

where $V_\omega = (X^T \Omega X + B^{-1})$ and $m_\omega = V_\omega (X^T \kappa + B^{-1} b)$, with $\Omega = \text{diag}\{\omega_1, \dots, \omega_n\}$ and $\kappa = (\omega_1 \log r_1 + (y_1 - r_1)/2, \dots, \omega_n \log r_n + (y_n - r_n)/2)$.

The adherence of this approximate posterior to the true posterior highly depends on the values of r_i , with larger values of r_i resulting in better approximations. However, when employing this result in posterior sampling, large values of r_i imply longer computation time due to the computational cost of sampling Pólya-gamma random variables with large parameters. Although the specific choice of r_i remains an open point—discussed later in Section 2.1.4—in the context of MCMC sampling, we propose to reduce the computational burden related to the sampling of n Pólya-gamma random

variables marginalizing the Gaussian distribution in (2.3) with respect to the related Pólya-gamma density conditioned on $\beta^{(t-1)}$, the last available β sampled. Since this marginalization is not in a closed form we introduce a second level of approximation of the true posterior. Specifically, we introduce $q(\beta \mid \beta^{(t-1)})$ a density that depends on $\beta^{(t-1)}$, defined as the first-order Taylor expansion of the marginalized Gaussian distribution, i.e.

$$q(\beta \mid \beta^{(t-1)}) = (2\pi)^{-p/2} \det(V_{E(\omega)})^{-1/2} \exp \left\{ -\frac{1}{2} (\beta - m_{E(\omega)})^T V_{E(\omega)}^{-1} (\beta - m_{E(\omega)}) \right\}, \quad (2.4)$$

where $V_{E(\omega)} = (X^T \Omega X + B^{-1})$, $m_{E(\omega)} = V_{E(\omega)} (X^T \kappa + B^{-1} b)$, $\Omega = \text{diag}\{E(\omega_1), \dots, E(\omega_n)\}$, $\kappa = (E(\omega_1) \log r_1 + (y_1 - r_1)/2, \dots, E(\omega_n) \log r_n + (y_n - r_n)/2)$, and for each $i = 1, \dots, n$ the conditional expectation of each ω_i is simply

$$E(\omega_i^*) = \frac{r_i + y_i}{2(x_i^T \beta^{(t-1)} - \log r_i)} \left(\frac{e^{x_i^T \beta^{(t-1)}} - r_i}{e^{x_i^T \beta^{(t-1)}} + r_i} \right),$$

or equivalently

$$\beta \mid \beta^{(t-1)} \sim N(m_{E(\omega)}, V_{E(\omega)}). \quad (2.5)$$

The above construction is eventually used as the building block of efficient Metropolis-Hastings and importance sampling algorithms, as described in the following sections.

2.1.2. Metropolis-Hastings sampler

We employ the above sampling mechanism as the proposal density in a Metropolis-Hastings algorithm. Consistent with this, at each iteration of the MCMC sampler, an additional step that accepts or rejects the proposed draw is introduced. Specifically, we assume that conditionally on the current state of the chain $\beta^{(t-1)}$, a new value β^* is sampled from (2.5). Then, the acceptance probability

$$\alpha(\beta^*, \beta^{(t-1)}) = \min \left\{ 1, \frac{\pi(\beta^* \mid y)}{\pi(\beta^{(t-1)} \mid y)} \frac{q(\beta^{(t-1)} \mid \beta^*)}{q(\beta^* \mid \beta^{(t-1)})} \right\}, \quad (2.6)$$

is evaluated to decide whether to accept or reject the proposed β^* , where $\pi(\beta^* \mid y)$ is the exact posterior distribution.

To compute the acceptance probability in (2.6), the forward and backward transition densities $q(\beta^* \mid \beta^{(t-1)})$ and $q(\beta^{(t-1)} \mid \beta^*)$ must be computed. Consistent with this, approximation (2.4) is particularly useful: without it, it would be necessary to compute the marginal density where the Pólya-gamma random variables are integrated out. However, the marginalization with respect to the Pólya-gamma density does not lead to a closed form expression; thus, the Metropolis-Hastings algorithm cannot be defined.

Clearly, for increasing r_i the proposal density (2.5) is closer to the true full conditional distribution; hence, the related acceptance rate will be higher, and the Metropolis-Hastings algorithm will be similar to a Gibbs sampler. On the other hand, setting this parameter to get a lower acceptance rate can result in smaller autocorrelation, and hence a better mixing (Robert and Casella, 2010). We discuss an approach to choose r_i balancing these two extremes in Section 2.1.4.

2.1.3. Adaptive importance sampler

The sampling mechanism (2.5) can also be exploited within the context of importance sampling, where the posterior expectation of a function of the parameter β , $E(h(\beta)) = \int h(\beta) \pi(\beta | y) d\beta$ is evaluated via Monte Carlo integration without direct sampling from $\pi(\beta | y)$. To this end, the general approach is to define an importance density $q(\beta)$ that is used to sample values $\beta^{(1)}, \dots, \beta^{(T)}$, which are eventually averaged to obtain an approximation of $E(h(\beta))$ through

$$\widehat{E(h(\beta))} = \frac{1}{T} \sum_{t=1}^T \tilde{w}(\beta^{(t)}) h(\beta^{(t)}),$$

with weights

$$\tilde{w}(\beta^{(t)}) = \frac{\pi(\beta^{(t)} | y)}{q(\beta^{(t)})}.$$

The efficiency of this algorithm is determined by the ability of the importance density to sample values relevant to the target density. To improve this aspect, we modify the original algorithm and, at each iteration, we simulate values from (2.5), updating the importance density with (2.4). Thus, the importance density is adaptively updated based on the previously extracted value $\beta^{(t-1)}$ and the weights become

$$\tilde{w}(\beta^{(t)}) = \frac{\pi(\beta^{(t)} | y)}{q(\beta^{(t)} | \beta^{(t-1)})}.$$

2.1.4. Tuning parameters r_i

The values of the parameters r_i , $i = 1, \dots, n$, have to be tuned to balance the trade-off between acceptance rate and autocorrelation in the Metropolis-Hastings, and to control the mixing of the weights in the importance sampler. However, tuning n parameters is not practical, especially for moderate to large n . The first simple solution sets all parameters equal to a single value r , however, in our experience, this resulted in a low effective sample size for some of the sampled chains.

As an alternative strategy, we choose to tune instead the distance of the proposal density from the target posterior. As the expression of the posterior distribution is unknown, we control the distance between the Poisson and negative binomial likelihood. Based on Teerapabolarn (2012), we consider the upper bound of the relative error between the Poisson and negative binomial cumulative distribution functions. This result is particularly useful owing to its simplicity, which allows to analytically derive adequate parameters to bound the error to a specific value. Specifically, if Y is a Poisson random variable with mean λ_i and V is a negative binomial random variable with parameters r_i and p_i , as defined in Section 2.1.1, we have the following result:

$$\sup_{y_i \geq 0} \left| \frac{\Pr(Y \leq y_i)}{\Pr(V \leq y_i)} - 1 \right| = e^{-\lambda_i} p_i^{-r_i} - 1.$$

Hence, by setting an upper bound d for the distance between the Poisson and negative binomial distribution, all the values of the parameters r_i can be automatically derived

to obtain a proposal density whose distance from the target posterior is constant for every y_i , even for heterogeneous data. Under our notation $p_i = \lambda_i/(r_i + \lambda_i)$, thus $d = e^{-\lambda_i}(1 + r_i/\lambda_i)^{r_i} - 1$, which is solved by

$$r_i = -\lambda \log c \cdot \left\{ \log c + \lambda \cdot W \left(\frac{-c^{-1/\lambda} \log c}{\lambda} \right) \right\}^{-1}, \quad (2.7)$$

where $c = e^\lambda(d^2 + 1)$ and $W(\cdot)$ is the Lambert-W function (Lambert, 1758), which can be computed numerically using standard libraries. Hence, in the algorithm, at the beginning of each iteration, the values r_1, \dots, r_n are computed according to (2.7) conditionally on the current value of β .

2.2. NUMERICAL ILLUSTRATIONS

2.2.1. Synthetic data

We conducted a simulation study under various settings to compare the efficiency of the proposed Metropolis-Hastings and importance sampler with that of state-of-the-art methods. We focused on the Hamiltonian Monte Carlo approach—as implemented in the Stan software (Stan Development Team, 2021)—as the successful Metropolis-Hastings with standard random walk proposal would require, different from the proposed approaches, the tuning of p parameters, which becomes cumbersome for moderate to elevate p . The proposed methods are implemented via the R package `bpr`, which is written in efficient C++ language exploiting the `Rcpp` package (Eddelbuettel and Francois, 2011) and available from the Comprehensive R Archive Network (D’Angelo, 2021) and in the repository at github.com/laura-dangelo/bpr.

Data were generated from a Poisson log-linear model with sample sizes $n \in \{25, 50, 100, 200\}$ and number of covariates $p \in \{5, 10, 20\}$. Specifically, for each combination of n and p , we consider 50 independent n dimensional vectors of counts where each y_i ($i = 1 \dots, n$) is sampled from a Poisson distribution with mean $\lambda_i = e^{x_i^T \beta}$, with common parameter β . The covariates were generated from continuous or discrete/categorical random variables under the constraints that the continuous variables have mean zero and variance one and that $1 \leq \lambda_i \leq 200$.

Two prior distributions for the coefficients β were assumed, namely a vanilla Gaussian prior with independent components $\beta_j \sim N(0, 2)$, $j = 1, \dots, p$, and the more complex horseshoe prior (Carvalho *et al.*, 2010) which allows for the following conditionally Gaussian representation

$$\begin{aligned} \beta_j &| \eta_j^2, \tau^2 \sim N(0, \eta_j^2 \tau^2) \\ \eta &\sim C^+(0, 1), \quad \tau \sim C^+(0, 1), \end{aligned}$$

for $j = 1, \dots, p$, where $C^+(0, 1)$ is the standard half-Cauchy distribution. To implement the samplers under the horseshoe prior, we used the details of Makalic and Schmidt (2016), and fixed the global shrinkage parameter τ to the “optimal value” $\tau_n(p_n) = (p_n/n)\sqrt{\log(n/p_n)}$, where p_n is the number of non-zero parameters (van der Pas *et al.*, 2017).

Each method introduced in Section 2.1 was run for 10000 iterations with 5000 of them discarded as burn-in. The convergence of each algorithm was assessed by graphical inspection of the trace plots of the resulting chains. The convergence was satisfactory for all simulations and comparable for all algorithms, as no systematic bias was found in the posterior mean of the estimated parameters.

To assess the efficiency of the proposed methods, we used a proxy of the time per independent sample, which is estimated as the total time (in seconds) necessary to simulate the entire chain, over the effective sample size of the resulting chain. For the proposed adaptive importance sampler, an estimate of the effective sample size was obtained using the quantity $\sum_{t=1}^T w(\beta^{(t)})^2 / (\sum_{t=1}^T w(\beta^{(t)}))^2$, which takes values between 1 and n (Robert and Casella, 2010). Notably, the burn-in samples were removed from the chains before computing the effective sample size. Thus, the obtained times per independent sample do not represent exactly the number of seconds necessary to generate one independent sample—they rather represent an overestimate. Nonetheless, this approach provides a robust and fair comparison between the different competing algorithms. The experiment has been run on a Linux machine with 8 GB DDR4 2400 MHz RAM, CPU Intel i7-7700HQ 3.8 GHz, running R 4.1.1.

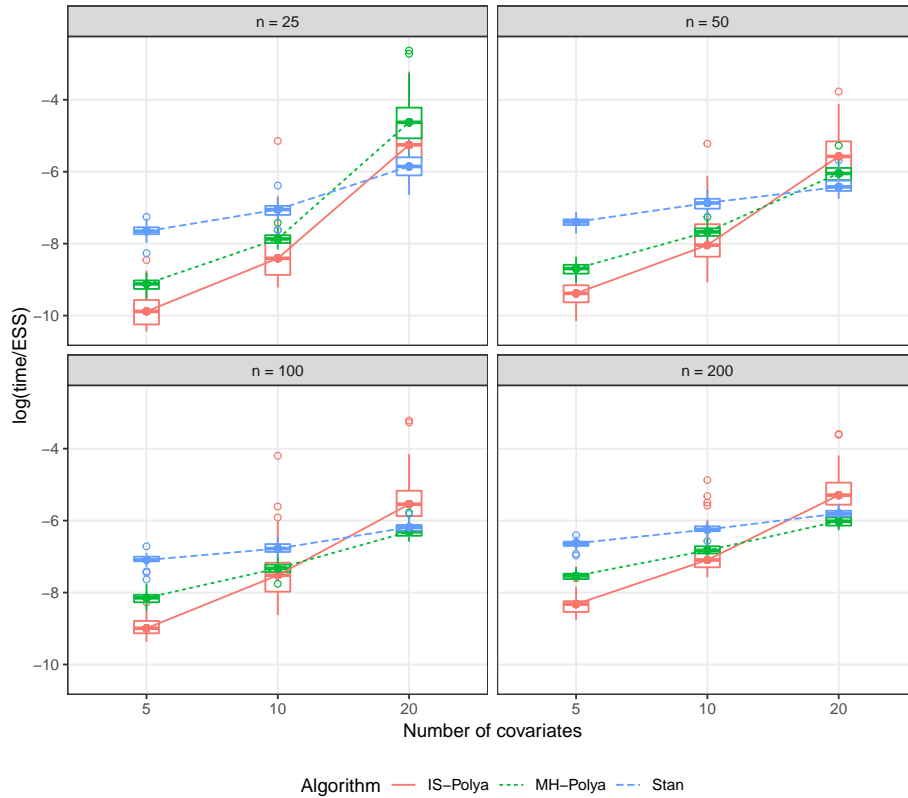


FIGURE 2.1: Time per independent sample (in logarithmic scale) for the three algorithms. For each combination of n and p the boxplots represent the distribution of the (log) time (in seconds) over the effective sample size using a Gaussian prior, over 50 replications.

Figure 2.1 and 2.2 show, for each combination of n and p , the distribution of the

median time per independent sample for the three algorithms computed on the 50 replications under a Gaussian and horseshoe priors, respectively. The plots are presented in the logarithmic scale for clarity.

For the Gaussian prior the performances of the proposed algorithms are better than those obtained using the HMC implemented in Stan, for small values of the dimension p . For $p = 20$, instead, the performances of the HMC are quite competitive with respect to the importance sampling and broadly comparable to the proposed efficient Metropolis-Hastings algorithm. Notably, the differences are less evident with increasing sample size.

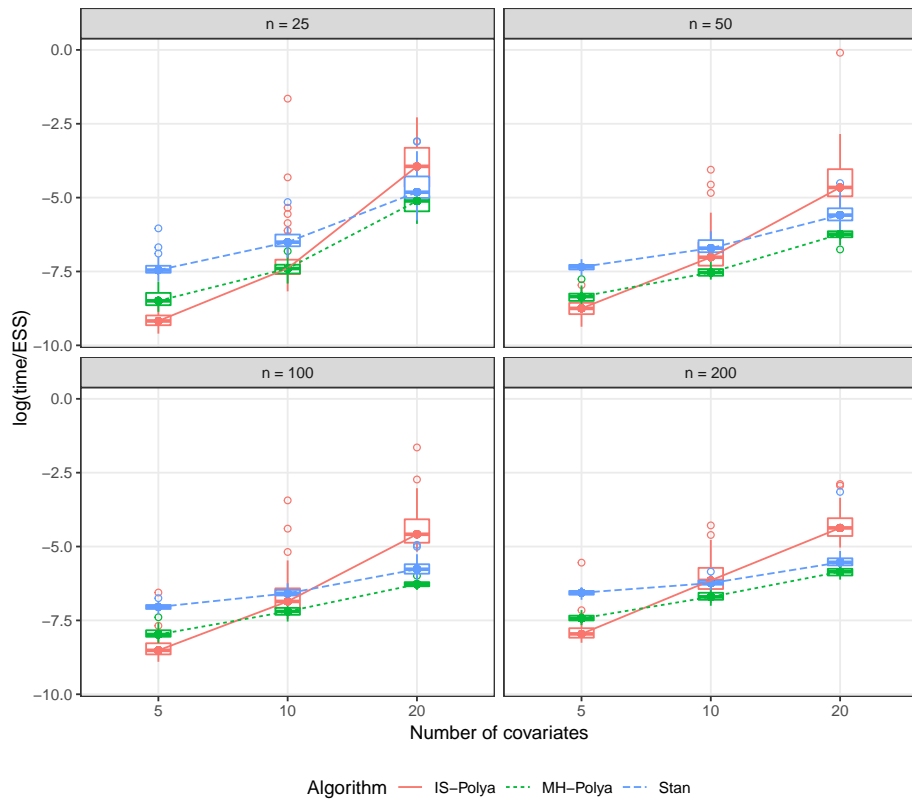


FIGURE 2.2: Time per independent sample (in logarithmic scale) for the three algorithms. For each combination of n and p the boxplots represent the distribution of the (log) time (in seconds) over the effective sample size using the horseshoe prior, over 50 replications.

For the horseshoe prior, the proposed Metropolis-Hastings presents a stable superior performance with respect to the HMC sampler implemented in Stan for each sample size n and number of covariates p . The performance of the importance sampler remains competitive. As previously observed for the Gaussian prior, the differences are less evident for increasing sample size.

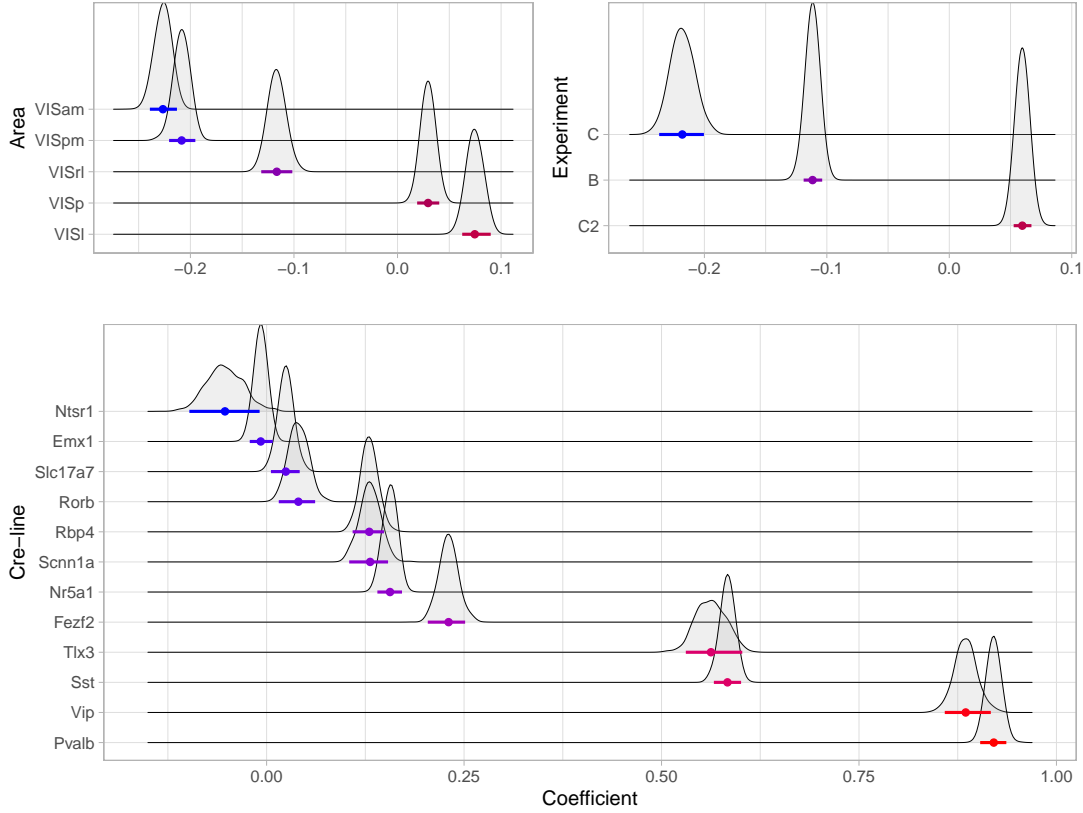


FIGURE 2.3: Coefficients of the regression on the calcium imaging data set: posterior density, with the posterior mean and 95% credible interval (colored dot and segment).

2.2.2. Spike train data

Herein, we illustrate the proposed sampling method on data of brain activity in mice in response to visual stimulation. The data set was generated using a small subset of data from the Allen Brain Observatory (Allen Institute for Brain Science, 2016), described in detail in Section 1.2.1. In the original data set, for each neuron the fluorescent calcium traces are recorded, which is a proxy of the neuronal activity, under different experimental conditions. From these traces, it is of interest to detect and analyze the activations of neurons, which correspond to transient spikes of the intracellular calcium level. We applied the method reported by Jewell *et al.* (2019) as described in de Vries *et al.* (2020) to extract and count the activations of each neuron, to understand how they are affected by the experimental conditions and the location of the neurons in the brain.

The covariates that we considered are the depth of the neuron, the area of the visual cortex where the neuron is located (factor with 6 levels), the cre transgenic mouse line (factor with 13 levels), and the type of visual stimulation (factor with 4 levels). The depth of the neurons is discretized to 22 levels, ranging from 175 to 625 microns, thus, we could obtain a data set having a full factorial design with 5 replications for each available covariate combination. Moreover, we included a quadratic term of the depth to improve the fitting. The obtained data set is made of 920 observations on 23

variables.

We ran the proposed Metropolis-Hastings algorithm for 9000 iterations, discarding the first 5000 as burn-in. The computation time was 98 seconds. The posterior estimates of the coefficients of the dummies on three categorical variables are shown in Figure 2.3; and for the numeric covariate depth, the posterior mean and 95% credible intervals were equal to -2.72×10^{-3} ($-2.90 \times 10^{-3}, -2.42 \times 10^{-3}$) for the linear term, and 5.59×10^{-6} ($5.11 \times 10^{-6}, 6.08 \times 10^{-6}$) for the quadratic term. Given these estimates of the coefficients, the number of spikes increased with the largest depths. Moreover, as shown in Figure 2.3, the response of neurons is heterogeneous across the cre-lines and, coherent with the results of de Vries *et al.* (2020), we obtained that the mean response is lower for the VISam, VISpm and VISrl areas.

3 | DECONVOLUTION AND MODELING OF CALCIUM IMAGING DATA WITH DISCRETE STIMULUS

As discussed in Section 1.1.2, routine methods to analyze calcium imaging data are based on a two-step approach. However, it is expected the rate and the distribution of spikes to be stimulus-dependent (Brenner *et al.*, 2002), but none of the previously described approaches allows to take into account explicitly the heterogeneity of spikes' behaviors as a function of the stimulus. As Figure 1.1 clearly shows for the Allen Brain Observatory data, the spikes' intensities vary greatly according to the type of stimulus.

In this chapter, we introduce a coherent nested Bayesian finite mixture model that allows for the estimation of the spiking activity of each neuron – which could be seen as a first step for the analysis of larger brain activity combining multiple neurons in a region. In addition, our model *simultaneously* allows for reconstructing the distributions of spikes under various experimental conditions; for example, in response to different types of visual stimuli in the Allen Brain Observatory data set.

More specifically, our modeling framework estimates and clusters the distributions of the calcium transient spikes' amplitudes via a nested formulation of the generalized mixture of finite mixtures (gMFM) prior recently proposed by Frühwirth-Schnatter *et al.* (2020). The proposed model further adopts the use of a common atom specification as in Denti *et al.* (2021) for estimating the distribution of the spikes' amplitudes under each experimental condition. The proposed common atom gMFM has several advantages with respect to typical Bayesian nonparametric models for nested data. With respect to models based on Dirichlet process priors, the gMFM provides increased flexibility to estimate partitions characterized either by many, well-balanced, clusters or by a small set of large clusters. The common atom model allows to obtain nested inference on densities without incurring in the degeneracy issues pointed out by Camerlenghi *et al.* (2019) for the widely used nested Dirichlet process of Rodríguez *et al.* (2008). At the same time, the common atom formulation still leverages two nested layers of random discrete mixture priors to borrow information between experiments and to identify similarities in the distributional patterns of the neuronal responses to different stimuli. In addition, differently than in the nested Dirichlet process, the common atom model also allows to cluster the inferred spikes' intensity values both within and between experimental conditions, so to infer common (recurring) response amplitudes. Finally, we allow our model to enforce sparsity of neuron firing over time by assuming a spike-and-slab prior specification on the marginal distribution of the amplitudes.

3.1. MODEL AND PRIOR SPECIFICATION

We consider the biophysical model for the calcium dynamics (1.1) introduced in Section 1.1.1, and the interpretation of the A_t parameters as *amplitude* of a spike at time t , taking value 0 if there is no spike and a positive value otherwise.

We are interested in characterizing the neuronal activity under different experimental conditions. For each time point $t = 1, \dots, T$, let g_t be a discrete categorical variable, taking values in $\{1, \dots, J\}$, where J is the number of distinct experimental settings, so that $g_t = j$ indicates that the neuronal activity at time t is observed under condition j . The experimental conditions are often designed to capture variations in neuronal activity with respect to a baseline process, which may represent a “typical” brain process. For example, in the Allen Observatory data, the interest is to investigate visually-evoked functional responses of neurons in the mouse’s visual cortex. Therefore, neurons associated with visual decoding should be expected to activate in all conditions. It is then of interest to study not only *if* but also *how* the neurons differentially respond to the presentation of a variety of visual stimuli.

In this chapter, we propose a hierarchical Bayesian approach to investigate similarities and differences in the distribution of spikes over time and conditions. In order to borrow information across different experimental conditions, one option is to fit a parametric hierarchical random effect model, and obtain a post-MCMC clustering of the estimated spikes A_t by grouping together those spikes with similar magnitudes. This approach has several limitations: on the one hand, the distribution of the random effects is constrained into a specific parametric form; on the other hand, the clustering of, say, the posterior mean estimates of the parameters A_t ’s does not allow to fully describe stimulus-specific distributional differences and to take into account the posterior uncertainty in the spikes.

In order to allow flexible modeling of distributions and to describe the heterogeneity of distributional features, we assume a nested Bayesian finite mixture specification. More specifically, we rewrite (1.1) as

$$y_t \mid b, \gamma, \text{Ca}_{t-1}, A_t, \sigma^2, \tau^2 \sim \text{N}(b + \gamma \text{Ca}_{t-1} + A_t, \sigma^2 + \tau^2)$$

and we assume that the spikes A_t are from stimulus-specific distributions, i.e. $(A_t \mid g_t = j, G_j) \sim G_j, j = 1, \dots, J$, to account for the observed variety of neuronal activity under different experiment settings. We further allow for clustering the distributions across conditions, in order to capture similar patterns of neuronal activity. Indeed, one may typically expect $K < J$ distributional clusters. For example, a neuron may respond to general visual stimulation and not specifically to the type of stimulus considered. More specifically, we assume the following generalized mixture of finite mixtures structure:

$$G_1, \dots, G_J \mid Q \sim Q, \quad Q = \sum_{k=1}^K \pi_k \delta_{G_k^*} \quad (3.1)$$

where $\pi_1, \dots, \pi_K \mid K \sim \text{Dirichlet}_K(\alpha/K, \dots, \alpha/K)$, $\alpha > 0$, and G_1^*, \dots, G_K^* are a set of cluster-defining distributions, obtained as realizations of an underlying random probability measure, specified further below. Equation (3.1) implies that the G_j ’s,

$j = 1, \dots, J$ have a positive probability of clustering together, thereby giving rise to *distributional clusters*. In practice, the number of mixture components, K , is typically larger than the number of clusters, K_+ , and some of the atoms G_k^* are not assigned to any of the G_j 's (empty components). The prior on the number of mixture components K is a translated beta-negative-binomial distribution as in Frühwirth-Schnatter *et al.* (2020). Including a prior $p(K)$ leads to both K_+ and K being random a priori. Finally, the distributional atoms G_k^* , $k = 1, \dots, K$ are also obtained as a realization from an underlying generalized mixture of finite mixtures,

$$G_k^* = \sum_{l=1}^L \omega_{l,k} \delta_{A_l^*} \quad (3.2)$$

with $\omega_{1,k}, \dots, \omega_{L,k} \mid L \sim \text{Dirichlet}_L(\beta/L)$, for some positive real number $\beta > 0$. The set of atoms A_l^* is common across all distributions G_1^*, \dots, G_K^* and they are obtained as i.i.d. draws from a centering measure, $A_l^* \sim G_0(A_l^*)$. Therefore, equation (3.2) defines a clustering of the inferred spike intensities both within a given condition (i.e. for fixed G_k^*) and across conditions (i.e. across the G_k^* 's; hence, across the G_j 's). In the following, we adopt common terminology in the literature on nested Bayesian non-parametric priors and indicate the clustering induced on the A_t through the proposed two-layers prior as *observational clustering*. The nested gMFM formulation requires the specification of a prior on the number of components that specify the lower-level distributional atoms G_k^* , $L \sim p(L)$. Once again, some of the components may be empty.

We enforce sparsity in the detection of the spikes by modeling the base measure G_0 for the parameters A_l^* with a spike-and-slab specification (Mitchell and Beauchamp, 1988), which is a convex mixture between a Dirac mass at zero – representing the absence of neuronal response – and a diffuse density on the positive real numbers – representing the intensity of the neuronal response. More specifically, we assume

$$G_0 = (1 - p) \delta_0 + p \text{Gamma}(h_{A1}, h_{A2}), \quad (3.3)$$

where the slab is a gamma distribution, $\text{Gamma}(a, b)$ with mean a/b and variance a/b^2 . The choice of a gamma distribution in (3.3) is particularly relevant for sparsity-inducing purposes, as the gamma density belongs to the set of moment non-local prior densities, as defined by Johnson and Rossell (2010). Therefore, a negligible probability density is assigned to values in a neighborhood of zero, thus inducing a clear separation between the baseline neuronal activity and the neuronal responses. In particular, the higher the shape parameter h_{A1} , the larger is the separation. We assume a $\text{Beta}(h_{1p}, h_{2p})$ prior for the proportion of spikes p with h_{1p} much smaller than h_{2p} in order to favor sparsity of detections.

The proposed formulation can be seen as a special case of *inner* spike-and-slab nonparametric priors, following a terminology introduced by Canale *et al.* (2017, 2021). In the following, we will refer to the proposed specification as a finite common atom model (fCAM).

The Bayesian model elicitation is completed by assuming conjugate priors for the underlying calcium level concentration parameters, i.e. the baseline calcium level b , and the variances σ^2 and τ^2 . Specifically, the following conjugate prior distributions

are assumed:

$$\begin{aligned} \text{Ca}_0 &\sim \text{N}(0, C_0), \quad b \sim \text{N}(b_0, B_0) \\ 1/\sigma^2 &\sim \text{Gamma}(h_{1\sigma}, h_{2\sigma}), \quad 1/\tau^2 \sim \text{Gamma}(h_{1\tau}, h_{2\tau}), \end{aligned}$$

Finally, under the assumption that the process is stationary with positive correlation between the calcium level at consecutive times, we constrain $\gamma \in (0, 1)$ and let $\gamma \sim \text{Beta}(h_{1\gamma}, h_{2\gamma})$, a priori.

3.2. POSTERIOR INFERENCE

For computational purposes, it is convenient to rewrite the likelihood for an observation y_t under condition $g_t = j$ by introducing two latent cluster allocation variables, $c_j^D = c_{g_t}^D$ and c_t , indicating the distributional cluster for the group j and the observational cluster for y_t , respectively.

Given K and $\{\pi_k\}_{k=1}^K$, the distributional allocation variable $c_j^D \in \{1, \dots, K\}$, with $\Pr(c_j^D = k) = \pi_k$. Similarly, conditionally on $c_{g_t}^D = k$, and given L and $\{\omega_{l,k}\}_{l=1}^L$, the observational allocation variable $c_t \in \{1, \dots, L\}$, with $\Pr(c_t = l) = \omega_{l,k}$. Therefore, conditionally on the other model parameters, the joint distribution of the observed data and the latent cluster allocations can be written as

$$f(\mathbf{y}, \mathbf{c}, \mathbf{c}^D \mid \boldsymbol{\pi}, \boldsymbol{\omega}, \mathbf{A}^*) = \prod_{j=1}^J \pi_{c_j^D} \prod_{t: g_t=j} \omega_{c_t, c_j^D} p(y_t \mid A_{c_t}^*),$$

which facilitates posterior inference.

More specifically, posterior inference for the proposed fCAM can be carried out quite straightforwardly by means of Markov chain Monte Carlo (MCMC) techniques. The sampling of the latent calcium level Ca_t uses an iterative approach based on the Kalman filter and on a forward filtering backward sampling algorithm (Prado and West, 2010). Full conditional posteriors for b , p , σ^2 and τ^2 are available in closed form thus leading to straightforward Gibbs sampling steps. For the autoregressive parameter γ , we use a Metropolis-Hastings within the Gibbs step. The sampling of A_t exploits a combination of the nested slice sampler of Denti *et al.* (2021) and of the telescoping sampler of Frühwirth-Schnatter *et al.* (2020). A detailed description of the latter step is reported in Algorithm 1 below. Here, we just present a schematic description of the MCMC steps:

- 1) Sample the calcium level Ca_t , for $t = 0, \dots, T$, using a forward filtering backward sampling:

- a) Run Kalman filter: set $a_0 = m_0 = 0$, $R_0 = C_0 = \text{var}(\text{Ca}_0)$. For $t = 1, \dots, T$ let

$$\begin{aligned} a_t &= \gamma m_{t-1} + A_t \\ R_t &= \gamma^2 C_{t-1} + \tau^2. \end{aligned}$$

Compute the filtering distribution's parameters, m_t and C_t , for $t = 1, \dots, T$, where

$$m_t = a_t + R_t (R_t + \sigma^2)^{-1} (y_t - b - a_t)$$

$$C_t = R_t - R_t^2 (R_t + \sigma^2)^{-1}.$$

b) Draw $\text{Ca}_T \sim \text{N}(m_T, C_T)$;

c) For $t = T - 1, \dots, 0$, draw $\text{Ca}_t \sim \text{N}(h_t, H_t)$, with

$$h_t = m_t + \gamma C_t R_{t+1}^{-1} (\text{Ca}_{t+1} - a_{t+1})$$

$$H_t = C_t - \gamma^2 C_t^2 R_{t+1}^{-1}.$$

2) Sample a new value for the baseline level b :

$$b \sim \text{N} \left(\frac{b_0}{B_0} + \frac{1}{\sigma^2} \sum_{t=1}^T (y_t - \text{Ca}_t), \sqrt{\frac{1}{B_0} + \frac{T}{\sigma^2}} \right).$$

3) Sample the variance on the output equation σ^2 and the variance on the state equation τ^2 :

$$1/\sigma^2 \sim \text{Gamma} \left(h_{1\sigma} + \frac{T}{2}, h_{2\sigma} + \frac{1}{2} \sum_{t=1}^T (y_t - \text{Ca}_t - b)^2 \right)$$

$$1/\tau^2 \sim \text{Gamma} \left(h_{1\tau} + \frac{T}{2}, h_{2\tau} + \frac{1}{2} \sum_{t=1}^T (\text{Ca}_t - \gamma \text{Ca}_{t-1} - A_t)^2 \right).$$

4) Update the autoregressive parameter γ using a Metropolis-Hastings step.

5) Update the parameter p of the spike-and-slab base measure from

$$p \sim \text{Beta}(h_{1p} + T - n_0, h_{2p} + n_0),$$

where n_0 is the number of y_t assigned to the the spike component.

6) Update the cluster allocations variables c^D and c , the number of mixture components K and L , and the cluster parameters \mathbf{A}^* using the nested telescoping sampling for the finite common atom model reported in Algorithm 1.

3.3. SIMULATION STUDY

The performances of the proposed method are assessed through a simulation study. The purpose of this section is twofold, namely to assess both the ability to correctly identify the spike times, and the accuracy of the inferred clustering structure.

We simulated synthetic data exhibiting a baseline level and a number of spikes representing the effect of the response of a neuron to a stimulus, thus mimicking the characteristics of real series of calcium imaging following the structure of model (1.1). Specifically, we first divided the time frame into J hypothetical experimental conditions of equal length, with J varying in the different scenarios described below. Consistent with our motivating assumption that the neuronal response depends on the type of

Algorithm 1 Nested telescoping sampling

Denote with \mathcal{C}^D the current partition on the distributions and with \mathcal{C}^O the partition on the observations.

- 1: Sample the weights on the distributions:

$$(\pi_1, \dots, \pi_K) \mid K, \alpha, \mathcal{C}^D \sim \text{Dirichlet}(e_1, \dots, e_K);$$

where $e_k = \alpha/K + J_k$, and J_k is the number of groups assigned to distribution k .

- 2: Sample the weights on the observations: for all $k \in \{1, \dots, K\}$ sample a vector ω_k from

$$(\omega_{1,k}, \dots, \omega_{L,k}) \mid L, \beta, \mathcal{C}^O, \mathcal{C}^D \sim \text{Dirichlet}(f_{1,k}, \dots, f_{L,k});$$

where $f_{l,k} = \beta/L + N_{l,k}$, and $N_{l,k}$ is the number of observations in the observational cluster l and distributional cluster k .

- 3: Update the partition on the distributions \mathcal{C}^D by sampling from the posterior distribution of the latent cluster allocation variables \mathbf{c}^D . For $j = 1, \dots, J$

$$\Pr(c_j^D = k \mid \pi, K, \mathbf{A}^*, \mathbf{y}, \mathbf{g}) \propto \pi_k \prod_{t: g_t = j} \omega_{c_t, c_j^D} p(y_t \mid A_{c_t}^*),$$

with $k \in \{1, \dots, K\}$. Determine $J_k = \#\{j : c_j^D = k\}$, for $k = 1 \dots, K$, and the number of non-empty components $K_+ = \sum_{k=1}^K I\{J_k > 0\}$. Relabel the components so that the first K_+ are non-empty.

- 4: Update the partition on the observations \mathcal{C}^O by sampling from the posterior distribution of the latent cluster allocation variables \mathbf{c} . For $t = 1, \dots, T$

$$\Pr(c_t = l \mid c_{g_t}^D = k, \mathbf{c}, \omega, L, K, \mathbf{A}^*, \mathbf{y}, \mathbf{g}) \propto \omega_{l,k} p(y_t \mid A_{c_t}^*),$$

with $l \in \{1, \dots, L\}$, $k \in \{1, \dots, K\}$. Determine $N_l = \#\{t : c_t = l\}$, for $l = 1 \dots, L$, and the number of non-empty components $L_+ = \sum_{l=1}^L I\{N_l > 0\}$. Relabel the components so that the first L_+ are non-empty. Because all the mixtures share the same atoms, the cluster parameters are sorted regardless of the distributional cluster allocation.

- 5: Sample the cluster parameters for the non-empty components: $p(A_l^* \mid -) \propto p(A_l^*) \prod_{t: c_t = l} p(y_t \mid A_l^*)$.
- 6: Conditional on \mathcal{C}^D , sample the number of components K of the mixture on distributions.
- 7: Conditional on \mathcal{C}^O , sample the number of components L of the mixtures on observations. If $L > L_+$, sample a new parameter A^* for the empty components from the prior distribution.
- 8: Update the hyperparameter α on the Dirichlet distribution on the mixture weights on distributions.
- 9: Update the hyperparameter β on the Dirichlet distribution on the mixture weights on observations.

The posterior distributions for steps 6-9 are given in Frühwirth-Schnatter *et al.* (2020).

stimulus, each experimental condition is assumed to belong to one of the K distributional clusters. Then, for each experimental condition, we generated the neuronal activity: first, we generated the presence or absence of a neuron response uniformly in time, where the spike probability can vary across groups. Then, conditionally on the obtained activations, we generated some additional spikes in a short subsequent interval, so that it is very likely to observe close or even successive spikes. In this way, the data mimic a real calcium imaging time series. Moreover, we are able to conduct a careful assessment of the ability of the model to distinguish the presence of a single high spike versus the convolution of several spikes in consecutive times. Finally, the values A_t , conditionally on their distributional cluster, are generated from one of the finite sets of spike amplitudes described below.

We simulated 50 independent data sets for each of the three scenarios described henceforth. In Scenario 1 we assumed $J = 6$ experimental conditions, generated from $K = 4$ distributional clusters. The spike amplitudes in the distributional clusters are $(0.35, 0.89, 1.15, 1.80, 2.20)$, $(0.65, 0.89, 1.40, 1.80)$, $(0.35, 0.65, 1.15)$, and $(0.35, 0.89, 1.60)$. Scenario 2 assumes $J = 4$ experimental conditions and $K = 3$ distributional clusters with spike amplitudes equal to $(0.3, 0.5, 0.7, 0.9, 1.1, 1.5)$, $(0.3, 0.9, 1.5, 1.8)$, and $(0.5, 0.9, 1.5)$. Finally, Scenario 3 sets $J = 5$ and $K = 3$ with the spike amplitudes in the distributional clusters being $(0.3, 0.5, 0.7, 0.9, 1.1)$, $(0.3, 0.9, 1.1, 1.3)$, and $(0.7, 0.9, 1.3)$. While in Scenario 1 the amplitudes of the spikes are quite large, spaced apart, and with the corresponding distributional clusters well distinct, in Scenario 3 the spike amplitudes are more homogeneous and more clustered in time. Scenario 2 represents an in-between situation. Hence, from the first to the last scenario, we are assuming an increasing degree of complexity. The R script generating these synthetic datasets is described in the Supporting Information.

The results attained by the proposed fCAM are compared to those obtained exploiting the common atom model (CAM) of Denti *et al.* (2021) – which provides a benchmark for the clustering of the spikes and the stimulus-specific distributions – and to those obtained with the L_0 penalization method of Jewell *et al.* (2019) and the L_1 penalization method of Friedrich *et al.* (2017), which provide a benchmark for the task of spikes' detection. For the latter two methods we have assumed complete knowledge of the autoregressive constant controlling the rate of the calcium decay, since we found that the results were quite sensitive to this estimate.

To assess the sensitivity of the proposed fCAM to the prior specification, we repeated the numerical experiment for different values of the hyperparameters h_{A1} and h_{A2} in (3.3). In particular, the shape parameter h_{A1} was supposed to play a key role in the detection of spikes. Keeping fixed the ratio h_{A1}/h_{A2} , the parameters were set equal to 3, 4, 6, and 8: a small value implies, *a priori*, less separation between zero and the distribution of the positive spikes while a large value corresponds to the opposite effect.

Focusing on the classification of each time point as a spike or not, Figure 3.1 summarizes the misclassification rate for all competing methods under the three scenarios. The results of the 50 replications are summarized using boxplots. For our fCAM, we report only the results obtained with $h_{A1} = h_{A2} = 8$ as those obtained for the other choices are essentially equivalent. The rates are small in absolute value and broadly comparable across the different methods, thus confirming that all the competing models are

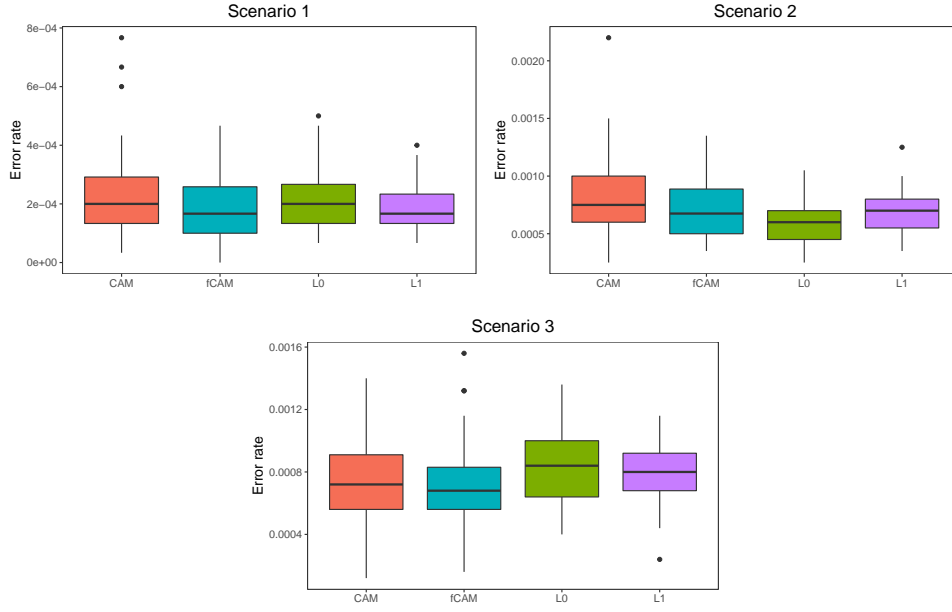


FIGURE 3.1: Distribution of the misclassification error rate in the simulation study for the four considered methods: CAM, fCAM, and the methods of Jewell *et al.* (2019) “L0” and Friedrich *et al.* (2017) “L1”.

effective in detecting the spikes.

However, the proposed fCAM not only enables the detection of spikes but also allows to conduct inference on the clustering structure. Therefore, we report on its ability to identify the clustering structure. Figure 3.2 reports the adjusted Rand index (Rand, 1971; Hubert and Arabie, 1985) computed on both the observational and the distributional clusters for $h_{A1} = h_{A2} = 8$ (results for other settings are similar). Values of the adjusted Rand index close to 1 denote that the identified structure resemble the true clustering. While for the observational clusters the results are broadly comparable, for the distributional clusters, the performance of the proposed fCAM is uniformly superior. In addition, the variability of the results generally appears to be drastically smaller for the fCAM, thus providing evidence of greater efficiency. This is consistent to the results of Frühwirth-Schnatter *et al.* (2020) where the generalized mixtures of finite mixtures is compared to a standard Dirichlet process mixture model.

From a computational point of view, the proposed algorithm is clearly more demanding than the optimization methods of Jewell *et al.* (2019) and Friedrich *et al.* (2017). However, the computing time is comparable to the slice sampler adopted for the CAM, and in general a full run requires just few minutes on a Linux machine with an i7-7700HQ 3.8 GHz Intel processor, 8 GB RAM, running R 4.1.0. For example, for a calcium trace of length 50,000, the computing time of the proposed method is around 2 minutes. Indeed, our experience suggests that the main factor affecting the computing time is the length of the series. In general, in the analysis of spike activity, we expect the number of clusters to be small and – in particular – much smaller than the number of observations.

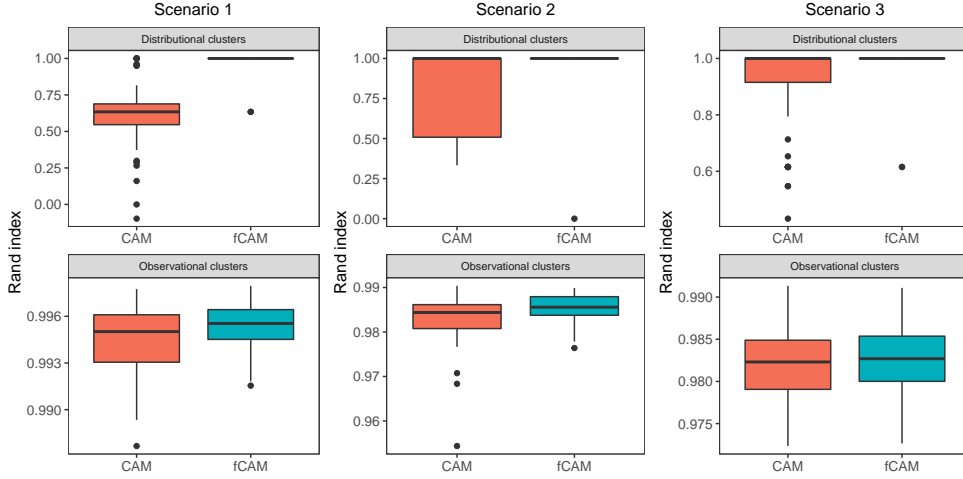


FIGURE 3.2: Distribution of the adjusted Rand index on the distributional and observational clusters, computed on the 50 simulations for the three scenarios of the simulated data.

3.4. ALLEN BRAIN OBSERVATORY DATA ANALYSIS

We now revert to the analysis of the data from the Allen Brain Observatory (Allen Institute for Brain Science, 2016). The data comprise the dF/F -transformed fluorescence trace for a cell during session-B of the experiment. This session comprises three types of visual stimuli (static gratings, natural scene and natural movie) in addition to some period of spontaneous activity (absence of visual stimuli). Since the data are recorded at a frequency of 30 Hz, the resulting series consists of 113,865 time points for a total of 63.2 minutes. We focus our analysis on a neuron located in the primary visual area, at an imaging depth equal to 350 microns. Additional analyses for other neurons are reported in the Supporting Information.

The observed fluorescence trace is shown with a continuous black line in Figure 3.3. Different shaded backgrounds indicate the types of visual stimuli. Using the notation introduced in the previous Sections, $J = 4$ with $j = 1, 2, 3$ corresponding to static grating, natural scene, and natural movie, respectively and $j = 4$ indicating no stimulus presence.

We ran the MCMC algorithm of Section 3.2 using the same prior specification of Section 3.1 for 15,000 iterations discarding the first 7,000 iterations as burn-in and keeping one iteration every four to improve mixing. Visual inspection of the traceplots and Geweke diagnostics showed no issues with convergence. The superimposed light line in Figure 3.3 represents the estimated neuronal activity in terms of the inferred amplitude A_t , i.e. removing the measurement errors and the result of the accumulation of calcium from the previous spikes. Here and henceforth, we identified the presence of a spike if the posterior probability of a spike at time t , say PPS_t , estimated by the proportion of non-zero A_t 's over all MCMC iterations, was greater than $\kappa = 75.5\%$. This threshold allows to control the (estimated) Bayesian false discovery rate at the

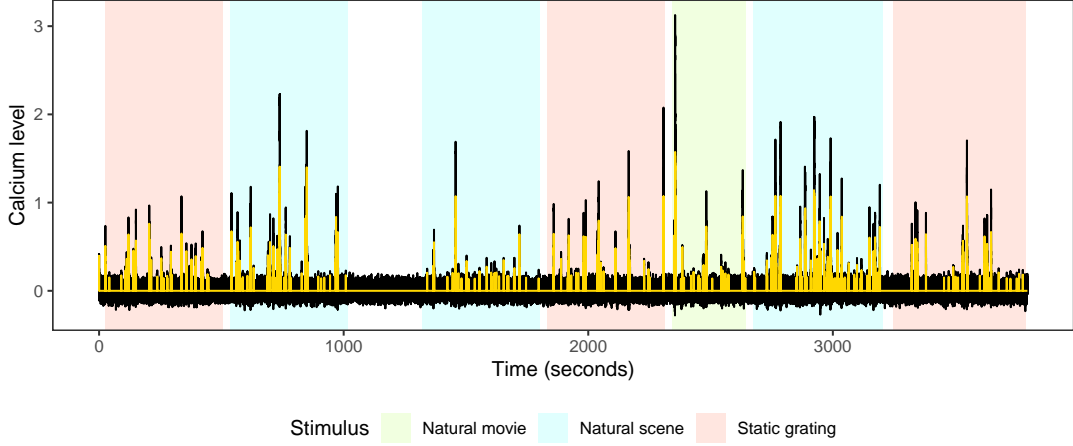


FIGURE 3.3: Observed fluorescence trace y_t from the Allen Brain Observatory data (black line), and visual stimulus to which the mouse is exposed (shaded areas). The yellow line represents the estimated neuronal activity.

pre-set value 0.05, that is κ solves the equation

$$\text{FDR}(\kappa) = \frac{\sum_{t=1}^T (1 - \text{PPS}_t) I_{(\text{PPS}_t > \kappa)}}{\sum_{t=1}^T I_{(\text{PPS}_t > \kappa)}} = 0.05.$$

For more details, we refer to Newton *et al.* (2004) and Müller *et al.* (2007). See also Sun *et al.* (2015) for a discussion with dependent hypotheses.

As already mentioned in the Introduction, in calcium imaging it is of interest studying the distribution of the spikes in response to each experimental stimulus, and identifying similarities and differences in these distributions across stimuli.

We start by investigating the presence of similarities in the neuronal response to different types of visual stimuli. This corresponds to analyzing the clustering of the spike distributions induced by the proposed fCAM. The model clusters together the groups corresponding to the natural scene and natural movie stimuli with high posterior probability, while the static grating stimulus and the absence of stimuli are assigned to two separate distributional clusters. In other terms, the neuron appears to show similar neuronal responses in the natural scene and natural movie stimuli whereas the responses appear distinctly different under the other two conditions.

To understand whether and how the neuronal response depends on the type of stimulus, we estimated the spike amplitude distribution for each of the four types of stimuli. Figure 3.4 shows the histograms of posterior means of the non-zero spike amplitudes for the three types of stimuli. The distribution for the time interval between 1018-1319 sec in Figure 3.3 (absence of stimuli) is not presented because no activity was detected. Despite the apparent similarities of the distributions in Figure 3.4, the second cluster of spike amplitude distributions (natural scene and natural movie) shows a heavier tail. Specifically, the highest observed cluster during the static grating stimulus (top plot) is centered at 1.06, while for the other two stimuli we obtained several higher values, with the largest cluster centered around 1.43.

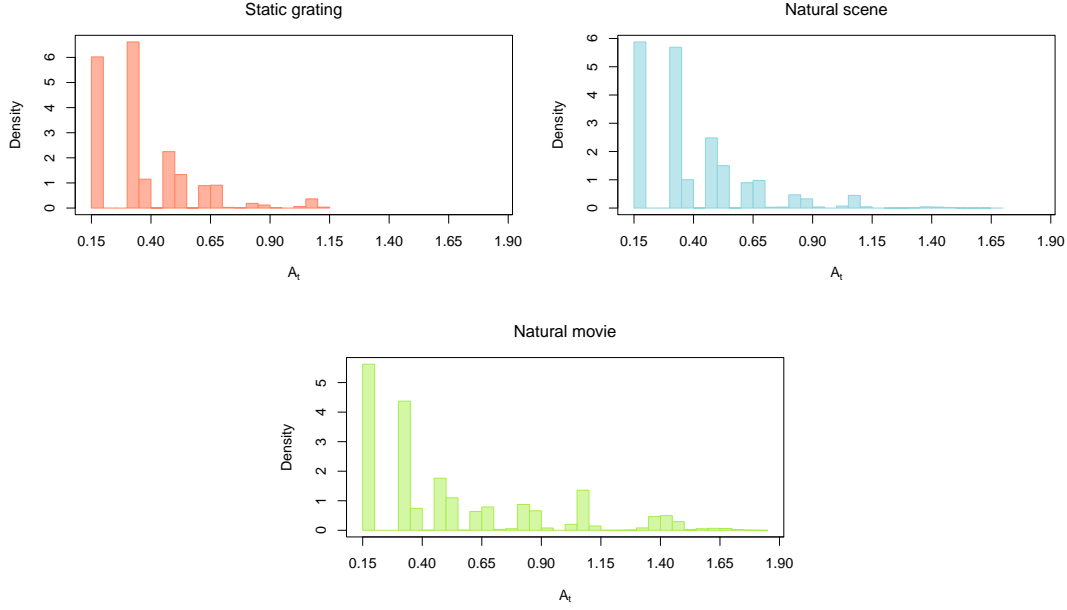


FIGURE 3.4: Empirical distribution of the posterior means of the observational cluster parameters A_t for the three experimental conditions of the Allen Brain Observatory data.

A qualitative representation of how these spike clusters are distributed within the three groups is given in Figure 3.5. The three plots show a short interval of the observed calcium series, chosen in correspondence of one of the highest observed spikes. Each plot also shows a series of colored vertical lines: the lines are placed at the estimated spike times, and the colors correspond to the estimated spike amplitudes. The represented partition is the posterior point estimate obtained by minimizing the variation of information loss, as proposed in Wade and Ghahramani (2018). Conditionally on the obtained partition, for each cluster a representative value for the cluster parameter is obtained as follows: first, for each MCMC iteration, the group-specific average of A_t is computed keeping the partition fixed; then, these values are averaged over all the MCMC iterations. We notice that for all experiments, high values of the observed calcium level are often produced as the result of several consecutive spikes, since, individually, the spikes are characterized by a relatively low amplitude, and the observed calcium level is cumulated due to its autoregressive behavior. The autoregressive parameter γ has a posterior mean equal to 0.493 with a 95% credible interval of (0.481, 0.505). This result corresponds to the understanding that the observed calcium response may be generated by high-frequency firing neurons: due to the low-sampling rate, the non-linear calcium signal essentially captures a super-imposition of multiple spikes (Hoang *et al.*, 2020).

As a matter of fact, another useful quantity we can compute to compare the neuronal activity between stimuli is the firing rate, which provides a measure of how often the neuron has activated during a specific visual stimulus. The rate computes the number of detected spikes per second, to take into account the different duration of the experiments. For the static grating stimulus the posterior mean rate (and related 95%

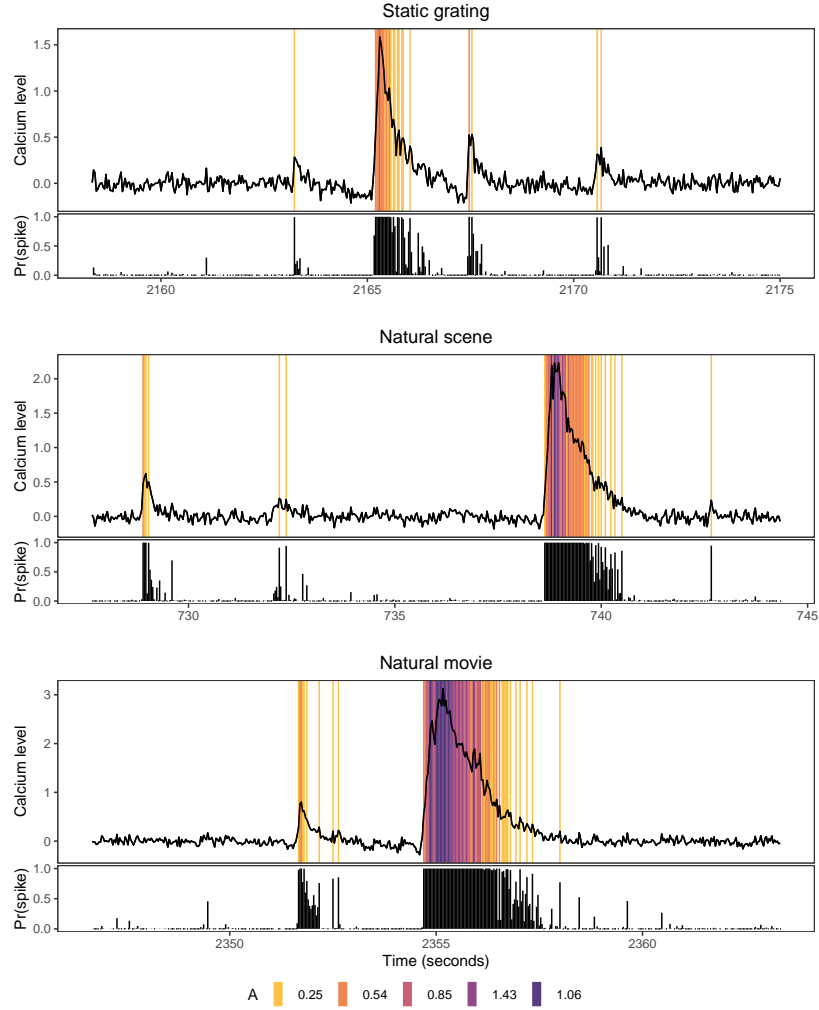


FIGURE 3.5: Short interval of length 500 of the Allen Brain Observatory data in correspondence of a spike, for the three stimuli. The vertical lines indicate the time of a spike and the colors correspond to the observational cluster of its amplitude. The bottom panels show the estimated posterior probability of spike presence, for each time point.

credible interval) is 0.223 (0.216, 0.229), while for the natural scene and natural movie stimuli they are 0.419 (0.410, 0.428) and 0.511 (0.495, 0.531), respectively. These results highlight the role of spike-frequency adaptation, whereby some neurons show an increased activity when exposed to more complex stimuli, thus exhibiting higher firing rates and larger calcium concentration measurements (Peron and Gabbiani, 2009).

CONCLUSIONS

DISCUSSION

ms.

FUTURE DIRECTIONS OF RESEARCH

A | APPENDIX NAME

BIBLIOGRAPHY

- Albert, J. H. and Chib, S. (1993) Bayesian analysis of binary and polychotomous response data. *Journal of the American Statistical Association* **88**(422), 669–679.
- Allen Brain Observatory (2017) Technical whitepaper: stimulus set and response analyses. Available at: <http://help.brain-map.org/display/observatory/Documentation>.
- Allen Institute for Brain Science (2016) Allen brain observatory. Available at: <http://observatory.brain-map.org/visualcoding>.
- Berridge, M. J., Lipp, P. and Bootman, M. D. (2000) The versatility and universality of calcium signalling. *Nature Reviews Molecular Cell Biology* **1**, 11 – 21.
- Blackwell, D. and MacQueen, J. B. (1973) Ferguson distributions via Polya urn schemes. *The Annals of Statistics* **1**(2), 353 – 355.
- Bradley, J. R., Holan, S. H. and Wikle, C. K. (2018) Computationally efficient multivariate spatio-temporal models for high-dimensional count-valued data (with discussion). *Bayesian Analysis* **13**(1), 253–310.
- Brenner, N., Agam, O., Bialek, W. and de Ruyter van Steveninck, R. (2002) Statistical properties of spike trains: universal and stimulus-dependent aspects. *Physical review. E, Statistical, nonlinear, and soft matter physics* **66**, 031907.
- Camerlenghi, F., Dunson, D. B., Lijoi, A., Prünster, I. and Rodríguez, A. (2019) Latent Nested Nonparametric Priors (with Discussion). *Bayesian Analysis* **14**(4), 1303 – 1356.
- Canale, A., Lijoi, A., Nipoti, B. and Prünster, I. (2017) On the Pitman–Yor process with spike and slab base measure. *Biometrika* **104**(3), 681–697.
- Canale, A., Lijoi, A., Nipoti, B. and Prünster, I. (2021) Inner spike and slab Bayesian nonparametric models. *arXiv:2107.10223*.
- Carvalho, C. M., Polson, N. G. and Scott, J. G. (2010) The horseshoe estimator for sparse signals. *Biometrika* **97**(2), 465–480.
- Chan, A. B. and Vasconcelos, N. (2009) Bayesian Poisson regression for crowd counting. In *2009 IEEE 12th International Conference on Computer Vision*, pp. 545–551.
- D’Angelo, L. (2021) bpr: Bayesian Poisson regression. URL: <https://CRAN.R-project.org/package=bpr>.

- Denk, W., Strickler, J. H. and Webb, W. W. (1990) Two-photon laser scanning fluorescence microscopy. *Science* **248**, 73–76.
- Denti, F., Camerlenghi, F., Guindani, M. and Mira, A. (2021) A common atoms model for the bayesian nonparametric analysis of nested data. *Journal of the American Statistical Association* pp. 1–12.
- Dombeck, D. A., Harvey, C. D., Tian, L., Looger, L. L. and Tank, D. W. (2010) Functional imaging of hippocampal place cells at cellular resolution during virtual navigation. *Nature Neuroscience* **13**, 1433 – 1440.
- Drouin, E., Piloquet, P. and Péréon, Y. (2015) The first illustrations of neurons by Camillo Golgi. *The Lancet Neurology* **14**(6), 567.
- Dudai, Y. (2004) The neurosciences: the danger that we will think that we have understood it all. In *The new brain sciences: perils and prospects*, eds S. Rose and D. Rees, pp. 167 – 180. Cambridge University Press.
- Eddelbuettel, D. and Francois, R. (2011) Rcpp: Seamless R and C++ integration. *Journal of Statistical Software, Articles* **40**(8), 1–18.
- Ferguson, T. S. (1973) A Bayesian analysis of some nonparametric problems. *The Annals of Statistics* **1**(2), 209 – 230.
- Ferguson, T. S. (1974) Prior distributions on spaces of probability measures. *The Annals of Statistics* **2**(4), 615 – 629.
- Friedrich, J. and Paninski, L. (2016) Fast active set methods for online spike inference from calcium imaging. In *Advances In Neural Information Processing Systems*, eds D. Lee, M. Sugiyama, U. Luxburg, I. Guyon and R. Garnett, pp. 1984 – 1992.
- Friedrich, J., Zhou, P. and Paninski, L. (2017) Fast online deconvolution of calcium imaging data. *PLOS Computational Biology* **13**(3), 1 – 26.
- Frome, E. L. (1983) The analysis of rates using Poisson regression models. *Biometrics* **39**(3), 665–674.
- Frome, E. L. and Checkoway, H. (1985) Use of Poisson regression models in estimating incidence rates and ratios. *American Journal of Epidemiology* **121**(2), 309–323.
- Frühwirth-Schnatter, S., Frühwirth, R., Held, L. and Rue, H. (2009) Improved auxiliary mixture sampling for hierarchical models of non-Gaussian data. *Statistics and Computing* **19**(479).
- Frühwirth-Schnatter, S. and Malsiner-Walli, G. (2019) From here to infinity: Sparse finite versus Dirichlet process mixtures in model-based clustering. *Advances in Data Analysis and Classification* **13**, 33 – 64.
- Frühwirth-Schnatter, S., Malsiner-Walli, G. and Grün, B. (2020) Generalized mixtures of finite mixtures and telescoping sampling.

- Frühwirth-Schnatter, S. and Wagner, H. (2006) Auxiliary mixture sampling for parameter-driven models of time series of counts with applications to state space modelling. *Biometrika* **93**(4), 827–841.
- Gelman, A., Carlin, J., Stern, H., Dunson, D., Vehtari, A. and Rubin, D. (2013) *Bayesian Data Analysis, Third Edition*. Chapman & Hall/CRC Texts in Statistical Science. Taylor & Francis.
- Grienberger, C. and Konnerth, A. (2012) Imaging calcium in neurons. *Neuron* **73**(5), 862 – 885.
- Hastings, W. K. (1970) Monte Carlo sampling methods using Markov chains and their applications. *Biometrika* **57**(1), 97–109.
- Hoang, H., Sato, M.-a., Shinomoto, S., Tsutsumi, S., Hashizume, M., Ishikawa, T., Kano, M., Ikegaya, Y., Kitamura, K., Kawato, M. and Toyama, K. (2020) Improved hyperacuity estimation of spike timing from calcium imaging. *Scientific Reports* **10**(1), 17844.
- Hubert, L. and Arabie, P. (1985) Comparing partitions. *Journal of Classification* **2**(336), 193 – 218.
- Hutchinson, M. K. and Holtman, M. C. (2005) Analysis of count data using Poisson regression. *Research in Nursing & Health* **28**(5), 408–418.
- Ishwaran, H. and James, L. F. (2001) Gibbs sampling methods for stick-breaking priors. *Journal of the American Statistical Association* **96**(453), 161–173.
- Jewell, S. and Witten, D. (2018) Exact spike train inference via L0 optimization. *The Annals of Applied Statistics* **12**(4), 2457 – 2482.
- Jewell, S. W., Hocking, T. D., Fearnhead, P. and Witten, D. M. (2019) Fast nonconvex deconvolution of calcium imaging data. *Biostatistics* **21**(4), 709–726.
- Johnson, V. E. and Rossell, D. (2010) On the use of non-local prior densities in Bayesian hypothesis tests. *Journal of the Royal Statistical Society: Series B (Statistical Methodology)* **72**(2), 143–170.
- Joshua, S. C. and Garber, N. J. (1990) Estimating truck accident rate and involvements using linear and Poisson regression models. *Transportation Planning and Technology* **15**(1), 41–58.
- Kalli, M., Griffin, J. and Walker, S. (2011) Slice sampling mixture models. *Statistics and Computing* **21**, 93 – 105.
- Karlis, D. and Meligkotsidou, L. (2005) Multivariate Poisson regression with covariance structure. *Statistics and Computing* **15**, 255–265.
- Lambert, D. (1992) Zero-inflated Poisson regression, with an application to defects in manufacturing. *Technometrics* **34**(1), 1–14.

- Lambert, J. H. (1758) Observations variae in mathesin puram. *Acta Helvetica, physico-mathematico-anatomico-botanico-medica* **3**, 128–168.
- Makalic, E. and Schmidt, D. F. (2016) A simple sampler for the horseshoe estimator. *IEEE Signal Processing Letters* **23**(1), 179–182.
- Malsiner-Walli, G., Frühwirth-Schnatter, S. and Grün, B. (2016) Model-based clustering based on sparse finite Gaussian mixtures. *Statistics and Computing* **26**, 303 – 324.
- McCullagh, P. and Yang, J. (2008) How many clusters? *Bayesian Analysis* **3**(1), 101 – 120.
- Miaou, S.-P. (1994) The relationship between truck accidents and geometric design of road sections: Poisson versus negative binomial regressions. *Accident Analysis & Prevention* **26**(4), 471–482.
- Miller, J. W. and Harrison, M. T. (2018) Mixture models with a prior on the number of components. *Journal of the American Statistical Association* **113**(521), 340 – 356.
- Mitchell, T. J. and Beauchamp, J. J. (1988) Bayesian variable selection in linear regression. *Journal of the American Statistical Association* **83**(404), 1023–1032.
- Mukamel, E. A., Nimmerjahn, A. and Schnitzer, M. J. (2009) Automated analysis of cellular signals from large-scale calcium imaging data. *Neuron* **63**(6), 747 – 760.
- Müller, P., Parmigiani, G. and Rice, K. (2007) FDR and Bayesian multiple comparisons rules. In *Bayesian Statistics 8*, eds J. Bernardo, M. Bayarri, J. Berger, A. Dawid, D. Heckerman, A. Smith and M. West. Oxford, UK: Oxford University Press.
- Neal, R. M. (2011) MCMC using Hamiltonian dynamics. *Handbook of Markov chain Monte Carlo* **2**(11), 2.
- Nelder, J. A. and Wedderburn, R. W. M. (1972) Generalized linear models. *Journal of the Royal Statistical Society. Series A (General)* **135**(3), 370–384.
- Newton, M. A., Noueiry, A., Sarkar, D. and Ahlquist, P. (2004) Detecting differential gene expression with a semiparametric hierarchical mixture method. *Biostatistics* **5**(2).
- Nobile, A. (2004) On the posterior distribution of the number of components in a finite mixture. *The Annals of Statistics* **32**(5), 2044 – 2073.
- Nobile, A. and Fearnside, A. (2007) Bayesian finite mixtures with an unknown number of components: the allocation sampler. *Statistics and Computing* **17**, 147 – 162.
- Paninski, L., Pillow, J. and Lewi, J. (2007) Statistical models for neural encoding, decoding, and optimal stimulus design. In *Computational Neuroscience: Theoretical Insights into Brain Function*, eds P. Cisek, T. Drew and J. F. Kalaska, volume 165 of *Progress in Brain Research*, pp. 493–507. Elsevier.
- Park, T. and Casella, G. (2008) The Bayesian lasso. *Journal of the American Statistical Association* **103**(482), 681–686.

- Parker, D. (2006) Complexities and uncertainties of neuronal network function. *Philosophical transactions of the Royal Society of London. Series B, Biological sciences* **361**(1465), 81 – 99.
- Parker, D. (2010) Neuronal network analyses: premises, promises and uncertainties. *Philosophical transactions of the Royal Society of London. Series B, Biological sciences* **365**(1551), 2315 – 2328.
- van der Pas, S., Szabó, B. and van der Vaart, A. (2017) Adaptive posterior contraction rates for the horseshoe. *Electronic Journal of Statistics* **11**(2), 3196 – 3225.
- Peron, S. P. and Gabbiani, F. (2009) Role of spike-frequency adaptation in shaping neuronal response to dynamic stimuli. *Biological cybernetics* **100**(6), 505–520.
- Piironen, J. and Vehtari, A. (2017) Sparsity information and regularization in the horseshoe and other shrinkage priors. *Electronic Journal of Statistics* **11**(2), 5018 – 5051.
- Pnevmatikakis, E., Merel, J., Pakman, A. and Paninski, L. (2013) Bayesian spike inference from calcium imaging data. In *In Signals, Systems and Computers*, pp. 349 – 353.
- Pnevmatikakis, E. A., Soudry, D., Gao, Y., Machado, T. A., Merel, J., Pfau, D., Reardon, T., Mu, Y., Lacefield, C., Yang, W., Ahrens, M., Bruno, R., Jessell, T. M., Peterka, D. S., Yuste, R. and Paninski, L. (2016) Simultaneous denoising, deconvolution, and demixing of calcium imaging data. *Neuron* **89**(2), 285 – 299.
- Polson, N. G., Scott, J. G. and Windle, J. (2013) Bayesian inference for logistic models using Pólya-gamma latent variables. *Journal of the American Statistical Association* **108**(504), 1339–1349.
- Prado, R. and West, M. (2010) *Time Series: Modeling, Computation, and Inference*. First edition. Chapman and Hall. ISBN 1420093363.
- Rand, W. M. (1971) Objective criteria for the evaluation of clustering methods. *Journal of the American Statistical Association* **66**(336), 846–850.
- Richardson, S. and Green, P. J. (1997) On Bayesian analysis of mixtures with an unknown number of components (with discussion). *Journal of the Royal Statistical Society: Series B (Statistical Methodology)* **59**(4), 731 – 792.
- Robert, C. and Casella, G. (2010) *Introducing Monte Carlo methods with R*. Springer.
- Rodríguez, A., Dunson, D. B. and Gelfand, A. E. (2008) The nested dirichlet process. *Journal of the American Statistical Association* **103**(483), 1131 – 1154.
- Sethuraman, J. (1994) A constructive definition of Dirichlet priors. *Statistica Sinica* **4**(2), 639 – 650.
- Stan Development Team (2021) Stan modeling language users guide and reference manual. URL: <http://mc-stan.org/>.

- Sun, W., Reich, B. J., Tony Cai, T., Guindani, M. and Schwartzman, A. (2015) False discovery control in large-scale spatial multiple testing. *Journal of the Royal Statistical Society: Series B (Statistical Methodology)* **77**(1), 59–83.
- Teerapabolarn, K. (2012) The least upper bound on the Poisson-negative binomial relative error. *Communications in Statistics - Theory and Methods* **41**(10), 1833–1838.
- Teh, Y. W., Jordan, M. I., Beal, M. J. and Blei, D. M. (2006) Hierarchical Dirichlet processes. *Journal of the American Statistical Association* **101**(476), 1566 – 1581.
- Vogelstein, J. T., Packer, A. M., Machado, T. A., Sippy, T., Babadi, B., Yuste, R. and Paninski, L. (2010) Fast nonnegative deconvolution for spike train inference from population calcium imaging. *Journal of Neurophysiology* **104**(6), 3691–3704.
- de Vries, S., Lecoq, J., Buice, M., Groblewski, P., Ocker, G., Oliver, M., Feng, D., Cain, N., Ledochowitsch, P., Millman, D., Roll, K., Garrett, M., Keenan, T., Kuan, C., Mihalas, S., Olsen, S., Thompson, C., Wakeman, W., Waters, J. and Koch, C. (2020) A large-scale standardized physiological survey reveals functional organization of the mouse visual cortex. *Nature neuroscience* **23**(1), 138–151.
- Wade, S. and Ghahramani, Z. (2018) Bayesian cluster analysis: point estimation and credible balls (with discussion). *Bayesian Analysis* **13**(2), 559–626.
- Walker, S. G. (2007) Sampling the Dirichlet mixture model with slices. *Communications in Statistics - Simulation and Computation* **36**(1), 45–54.
- Wei, X.-X., Zhou, D., Grosmark, A., Ajabi, Z., Sparks, F., Zhou, P., Brandon, M., Losonczy, A. and Paninski, L. (2019) A zero-inflated gamma model for post-deconvolved calcium imaging traces .

Laura D'Angelo

CURRICULUM VITAE

Contact Information

University of Padova
Department of Statistics
via Cesare Battisti, 241-243
35121 Padova. Italy.

Tel. +39 049 827 4168
e-mail: laura.dangelo.1@phd.unipd.it

Current Position

Since October 2018; (expected completion: December 2021)

PhD Student in Statistical Sciences, University of Padova.

Thesis title: titletitle...

Supervisor: Prof. Antonio Canale

Co-supervisor: Prof. Michele Guindani.

Research interests

- Statistical modeling
- Bayesian statistics
- Bayesian nonparametrics
- Computational statistics

Education

October 2015 – November 2017

Master's (laurea specialistica/magistrale) degree in Statistical Science .

University of Padova, Department of Statistics

Title of dissertation: "Modelli Bayesiani nonparametrici: applicazioni al settore assicurativo "

Supervisor: Prof. Antonio Canale

Final mark: 110/110 cum laude.

October 2012 – September 2015

Bachelor's degree (laurea triennale) in Statistics, Economics and Finance.

University of Padova, Department of Statistics

Title of dissertation: "L'area sotto la curva ROC specifica per caratteristiche"

Supervisor: Prof. Gianfranco Adimari

Final mark: 110/110 cum laude.

Visiting periods

January 2020 – November 2020

University of California, Irvine;

Irvine, CA (USA).

Supervisor: Prof. Michele Guindani.

Work experience

January 2018 – September 2018

BIP S.p.A..

Consultant, data analyst.

Awards and Scholarship

July 2021 - ISBA 2021 World Meeting.

ISBA 2021 Best Student/Postdoc Contributed Paper Award.

Computer skills

- R (advanced)
- C++, GitHub, Python (working level)

Language skills

Italian: native;

English: fluent.

Publications

Articles in journals

D'Angelo L. and Canale A. (2021) Contributed Discussion on: “Centered partition processes: informative priors for clustering”, in *Bayesian Analysis*, **16**(1), 356–358.

D'Angelo L., Canale A., Yu Z. and Guindani M. (2021) Detection of neural activity in calcium imaging data via Bayesian mixture models, in *Book of Short Papers SIS 2021* (Editors: Perna C., Salvati N., Schirripa Spagnolo F.), ISBN: 9788891927361.

D'Angelo L. (2019) Model based clustering in group life insurance via Bayesian nonparametric mixtures, in *Book of Short Papers SIS 2019* (Editors: Arbia, G., Peluso, S., Pini, A. and Rivellini, G.), ISBN: 978889191510.

Working papers

D'Angelo L., Canale A., Yu Z. and Guindani M. (2021) Bayesian nonparametric analysis for the detection of spikes in noisy calcium imaging data. *arXiv preprint arXiv:2102.09403*

Conference presentations

D'Angelo L., Canale A., Yu Z. and Guindani M. (2021). Bayesian nonparametric analysis for the detection of spikes in noisy calcium imaging data. (contributed talk) *JSM 2021*, August 8 - 12, 2021.

D'Angelo L., Canale A., Yu Z. and Guindani M. (2021). Bayesian nonparametric analysis for the detection of spikes in noisy calcium imaging data. (contributed talk) *ISBA 2021 World Meeting*, June 23 - July 2, 2021. Pre-recorded video available at <https://youtu.be/SLLSJVuFnMs> .

D'Angelo L., Canale A., Yu Z. and Guindani M. (2021). Detection of neural activity in calcium imaging data via Bayesian mixture models. (contributed talk) *SIS 2021 Intermediate meeting*, Pisa, Italy, June 21 - 25, 2021.

D'Angelo L. (2019). Model based clustering in group life insurance via Bayesian nonparametric mixtures. *SIS 2019 Intermediate meeting*, Milan, Italy, June 12-14, 2019.

Teaching experience

April 2021

Tirocinio formativo

use of Latex for scientific writing, 2.5 hours

University of Padova

Other Interests

Member of LIPU (Lega Italiana Protezione Uccelli) since 2019.

Volunteer for the project Lipu LIFE Choo-na in 2019.

References

Prof. Antonio Canale

University of Padova

via Cesare Battisti, 241-243;
35121 Padova. Italy.

Phone: +39 049 827 4168

e-mail: canale@stat.unipd.it

Prof. Michele Guindani

University of California, Irvine

Donald Bren School of Information and Computer Sciences; Irvine, CA 92697-1250

Phone: +1 949 824 3276

e-mail: michele.guindani@UCI.edu