

CSG Meeting: fMRI pipelines comparison and process enhancement



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Outline

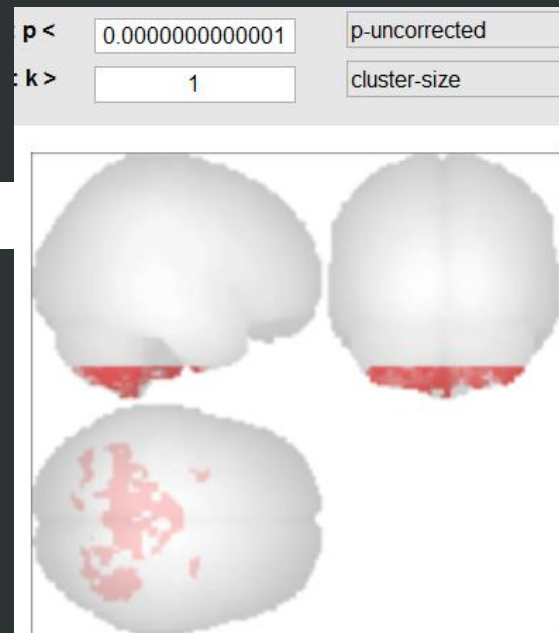
2

- FMRI pipeline comparison:
 - Code analysis
 - Segmentation
 - Denoising
 - First-level
 - Second-level
- Other considerations:
 - Threshold tweaking
 - Others (manips, etc)
- Conclusion

Background: Why?

Issues identified in new pipeline:

1. **Cerebellum artefact** →
2. **Signal shape tampered**, only noise remains (easy to spot on CONN Denoising and 1st-level previsualizations when compared to other pipelines)
3. **Controls were preprocessed with a different pipeline** (no idea which one, can be as old as Lizette's SPM8 pipeline).
4. Current pipeline **not validated** (uses NewSeg).



fMRI pipelines: Code analysis overview

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- Code & batch comparison using KDiff3 + manual inspection
- **7 packages (total: 18 pipelines scripts)** reviewed:
 1. Stephen's
 2. Athena's script for classifier
 3. Athena's script for cosmonauts
 4. Athena's from Charlène computer
 5. Lizette's
 6. Carol's
 7. Charlène's FMRI+PET scripts (latest used as of 06/2017)
- Each package contained 1 to 6 different pipelines with an average = 3.
“Athena's only” average = 1, “rest only” average = 4.

fMRI pipelines: Code analysis results

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- Analysis goal: **Isolate major differences** and ignore cosmetic changes (eg, different directories layout, non-critical parameters such as filepaths or TR due to migration)
- Significant changes included different versions of softwares (SPM8 vs SPM12, with or without VBM8/DARTEL, etc.), different modules versions (OldSeg vs NewSeg), critical parameters changes (eg, using another TPM template) and pipeline format (code+batch vs code only).

4 different scripts families were isolated:

1. SPM8 script no batch (Lizette, 2015?, Spatial_processing_Lizette*.m)
2. **SPM8+VBM8/DARTEL with batch** (Carol, 2016, script_preproc_VBM_Dartel_DEF*.m).
Note: Charlene has a variant VBM8+PET.
3. **SPM12 OldSeg with batch** (Athena, 2016-2017, script_preproc_LIE_spm12.m)
4. **SPM12 NewSeg CRC12 tpm+PET with batch** (Charlène, 2017, script_preproc_SPM12_Charlene.m)

Note: for the rest of this presentation, only scripts 2, 3 and 4 will be used

fMRI pipelines: Code analysis results

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- **SPM12 OldSeg (Athena's)** script is the **most stable** (in terms of code): always the same in all instances analyzed.
Pro: very fast, should fit most functional analyses + classifier.
- **3 different templates:**
 - spm8 Dartel custom patients template
 - spm12 no template (use standard)
 - spm12-NewSeg uses CRC12 custom template.
- Several **inconveniences** :
 - difficult to migrate (all templates and software paths hardcoded or hidden in batch)
 - easily breakable (PATH with multiple software versions, no apriori check of TR, of files existence, etc.)
→ script stops in the middle of preprocess instead of before
 - accents and long filenames unsupported and no check
 - 4d nifti unsupported

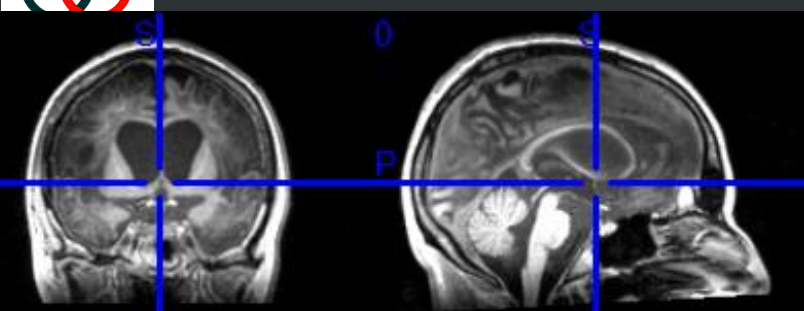
fMRI pipelines: Images comparisons

7

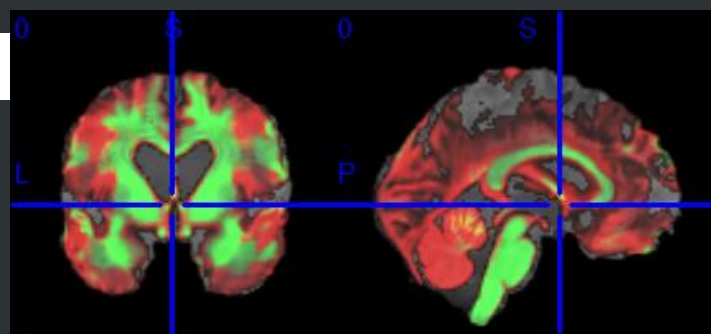
- Additional technical notes with the companion .txt file (with all equivalences).
- Now the boring part is done, we can check the resulting images with each pipeline 😊



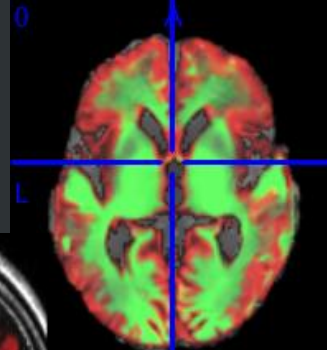
fMRI pipelines: Segmentation



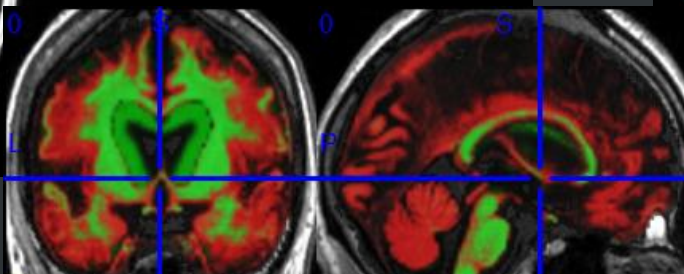
T1 original



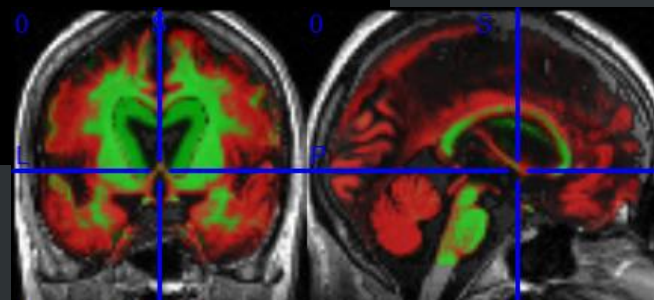
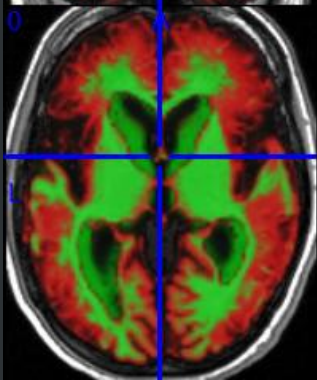
SPM8+VBM



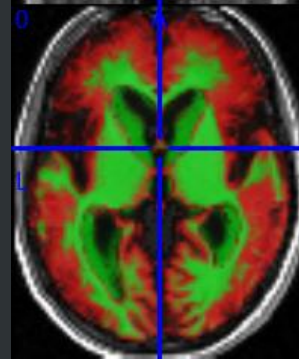
Notice →
the
Cerebellum
Cut!



SPM12
OldSeg



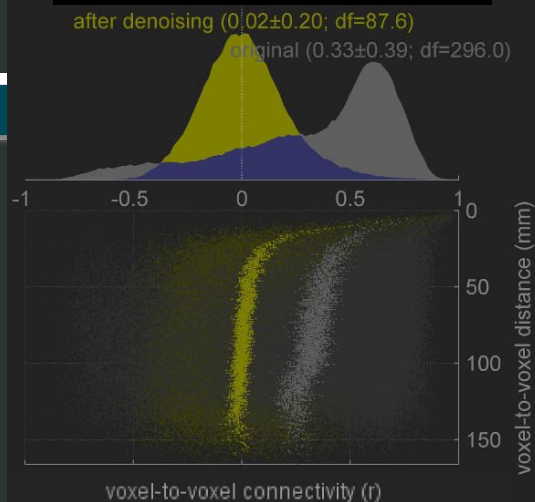
SPM12
NewSeg



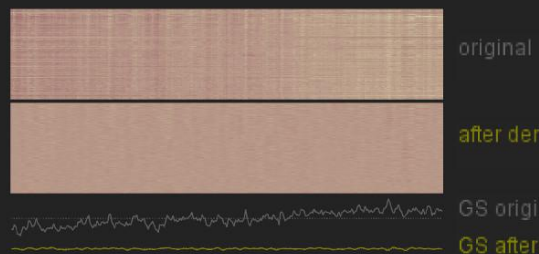
fMRI pipelines: Denoising Controls

SPM8+VBM

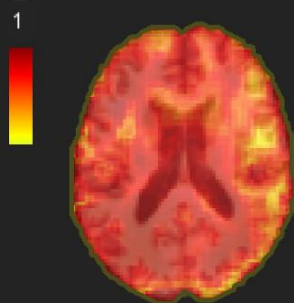
after denoising (0.02 ± 0.20 ; $df=87.6$)
original (0.33 ± 0.39 ; $df=296.0$)



BOLD timeseries

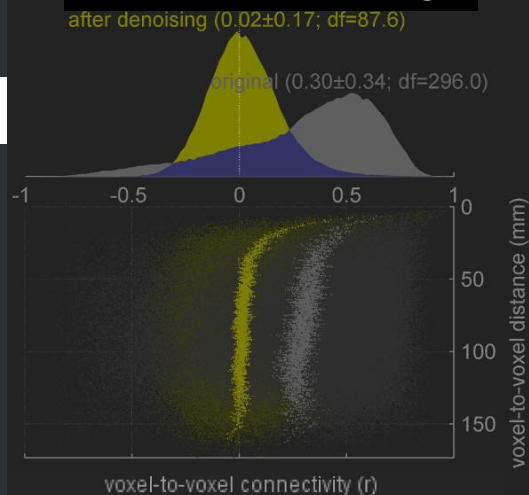


BOLD % variance explained by TOTAL

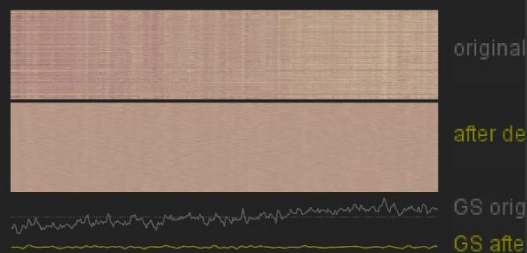


SPM12 OldSeg

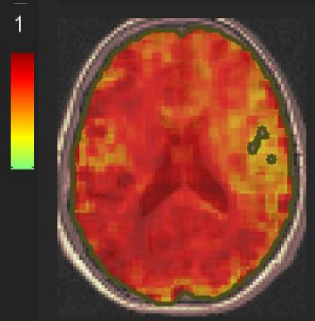
after denoising (0.02 ± 0.17 ; $df=87.6$)
original (0.30 ± 0.34 ; $df=296.0$)



BOLD timeseries

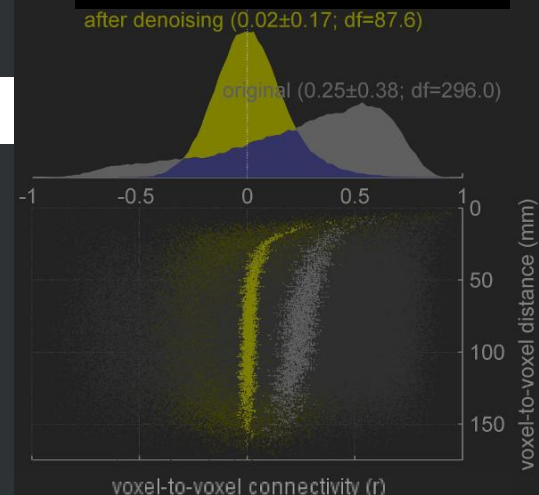


BOLD % variance explained by TOTAL

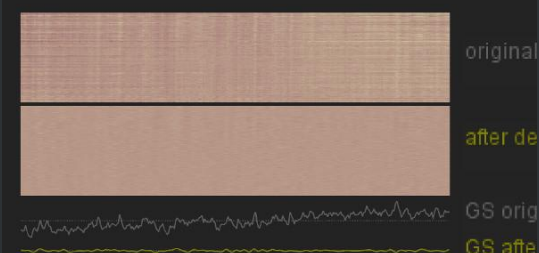


SPM12 NewSeg

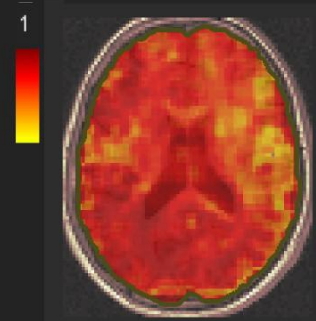
after denoising (0.02 ± 0.17 ; $df=87.6$)
original (0.25 ± 0.38 ; $df=296.0$)



BOLD timeseries



BOLD % variance explained by TOTAL

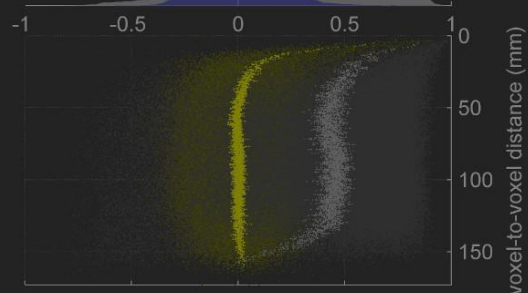


fMRI pipelines: Denoising Patient

SPM8+VBM

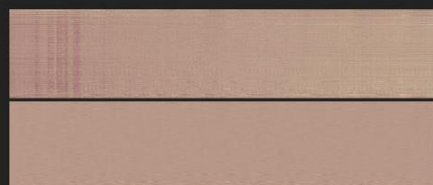
after denoising (0.01 ± 0.14 ; $df=86.3$)

original (0.44 ± 0.33 ; $df=296.0$)



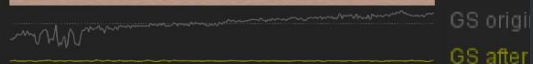
voxel-to-voxel connectivity (r)

BOLD timeseries

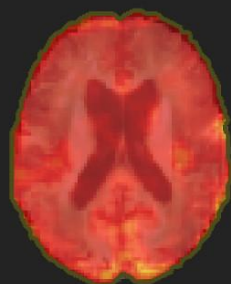


original

after denoising



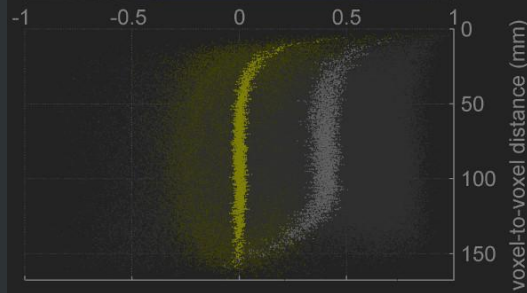
BOLD % variance explained by
TOTAL



SPM12 OldSeg

after denoising (0.01 ± 0.14 ; $df=86.3$)

original (0.39 ± 0.31 ; $df=296.0$)



voxel-to-voxel connectivity (r)

BOLD timeseries

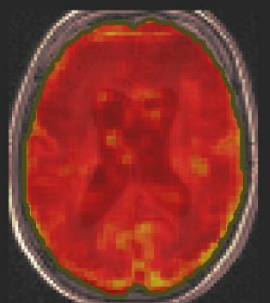


original

after denoising



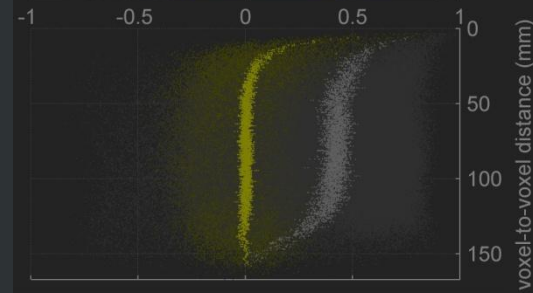
BOLD % variance explained by
TOTAL



SPM12 NewSeg

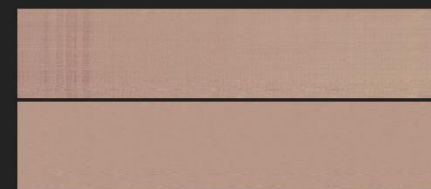
after denoising (0.01 ± 0.14 ; $df=86.3$)

original (0.41 ± 0.31 ; $df=296.0$)



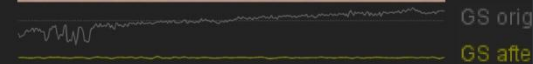
voxel-to-voxel connectivity (r)

BOLD timeseries

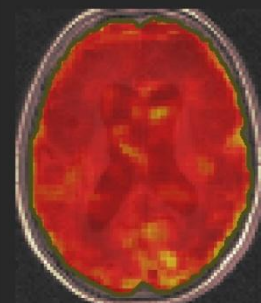


original

after denoising



BOLD % variance explained by
TOTAL

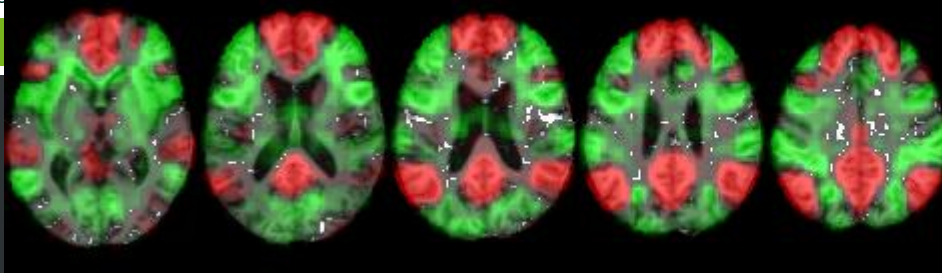




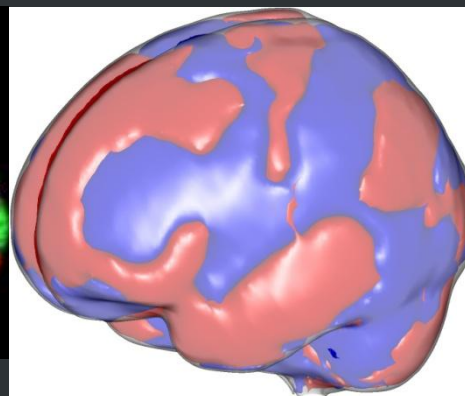
fMRI pipelines: First-Level Controls

(averaged on all 8 controls)

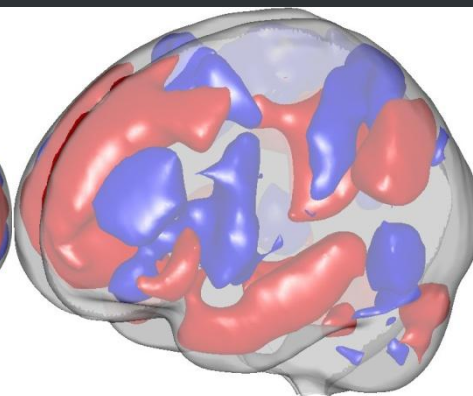
SPM8+VBM



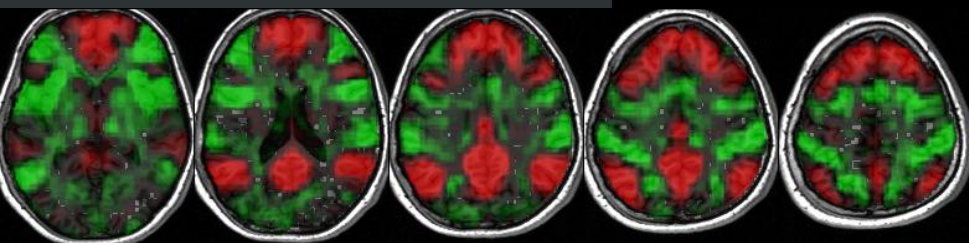
Binarized



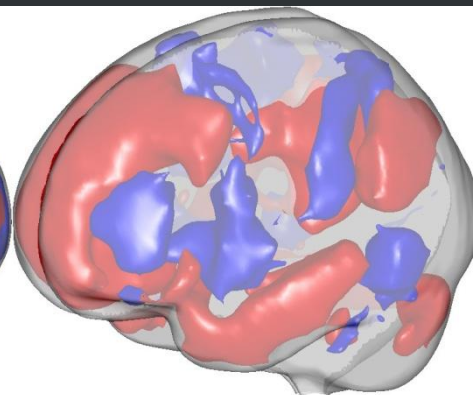
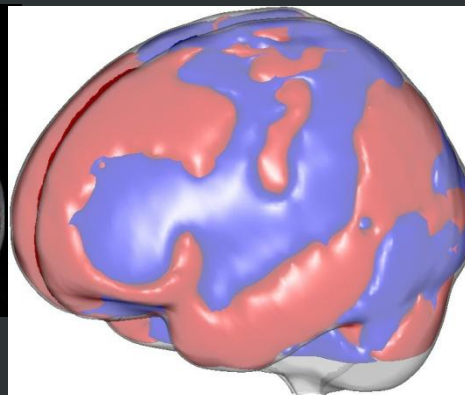
Threshold $Z \geq 0.1$



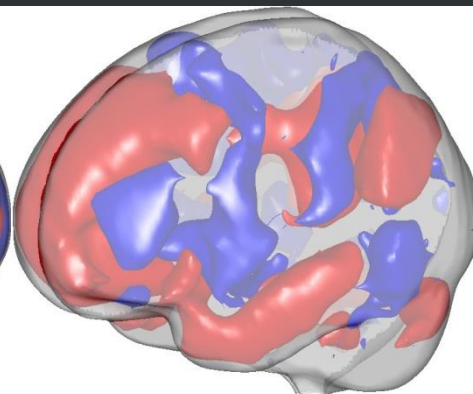
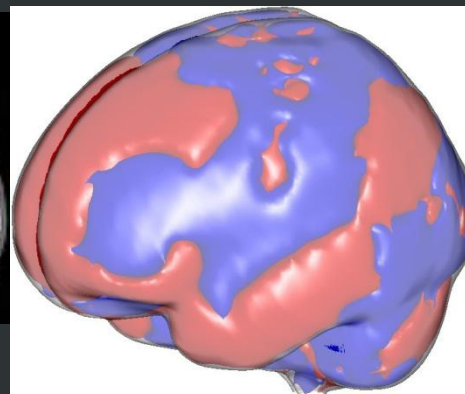
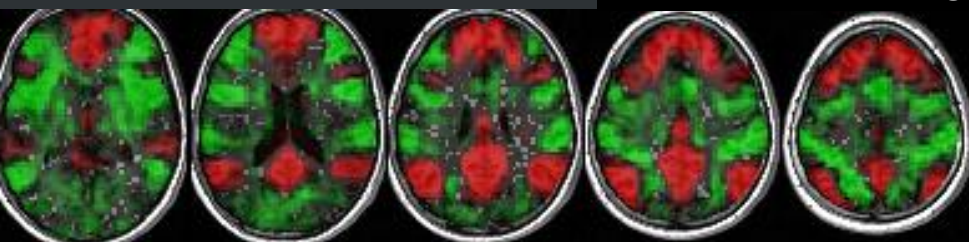
SPM12 OldSeg



Cerebellum cut again! →



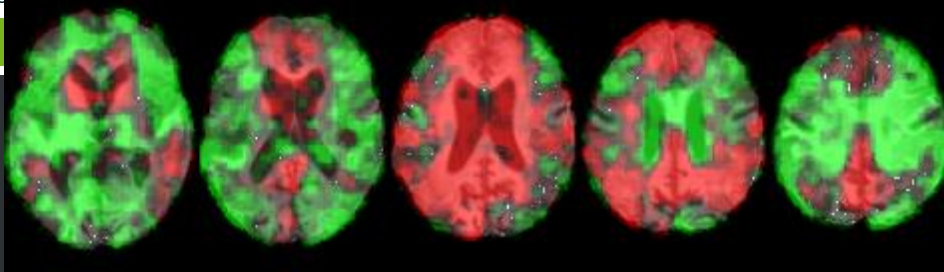
SPM12 NewSeg



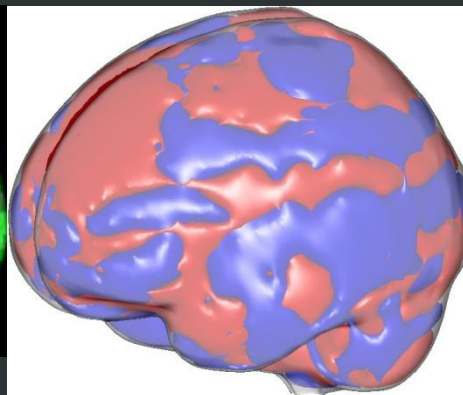


fMRI pipelines: First-Level Patient

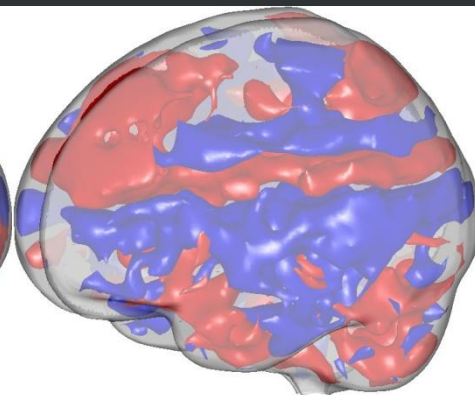
SPM8+VBM



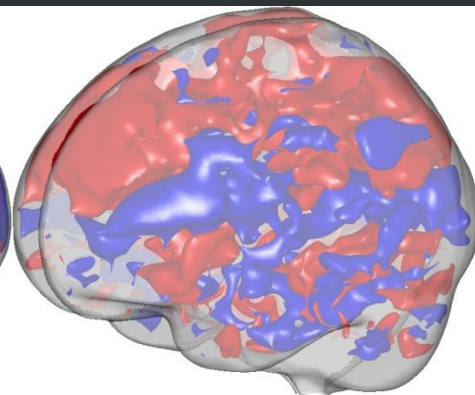
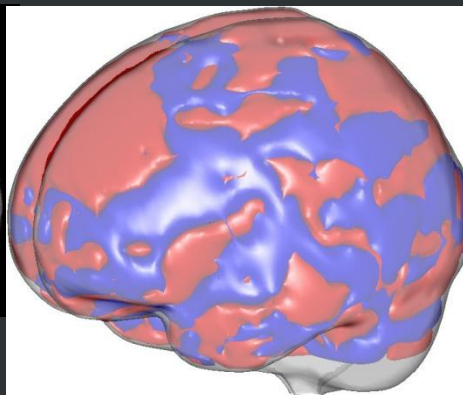
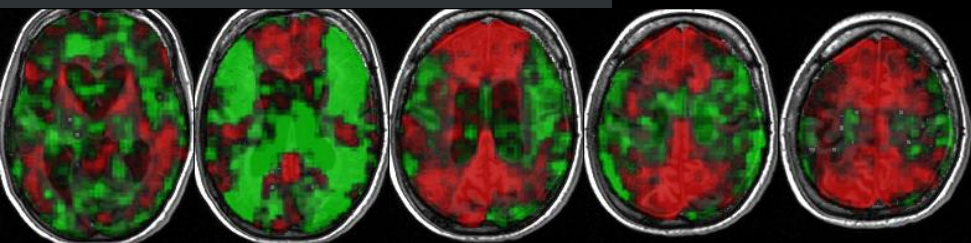
Binarized



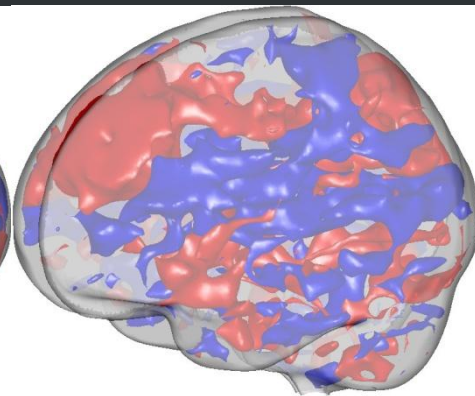
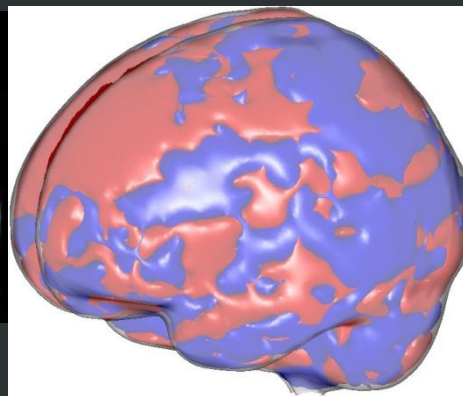
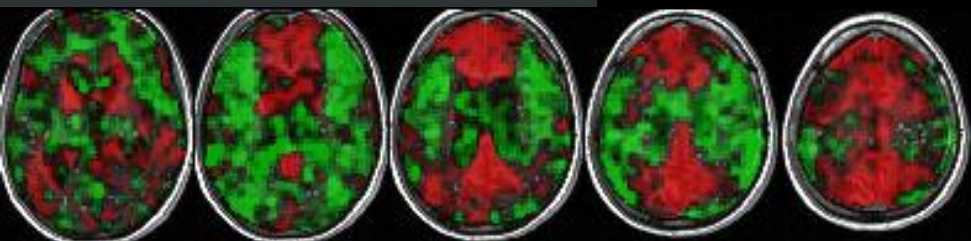
Threshold $Z \geq 0.1$



SPM12 OldSeg



SPM12 NewSeg



fMRI pipelines: Second-Level

Pipeline

Group

SPM8+VBM

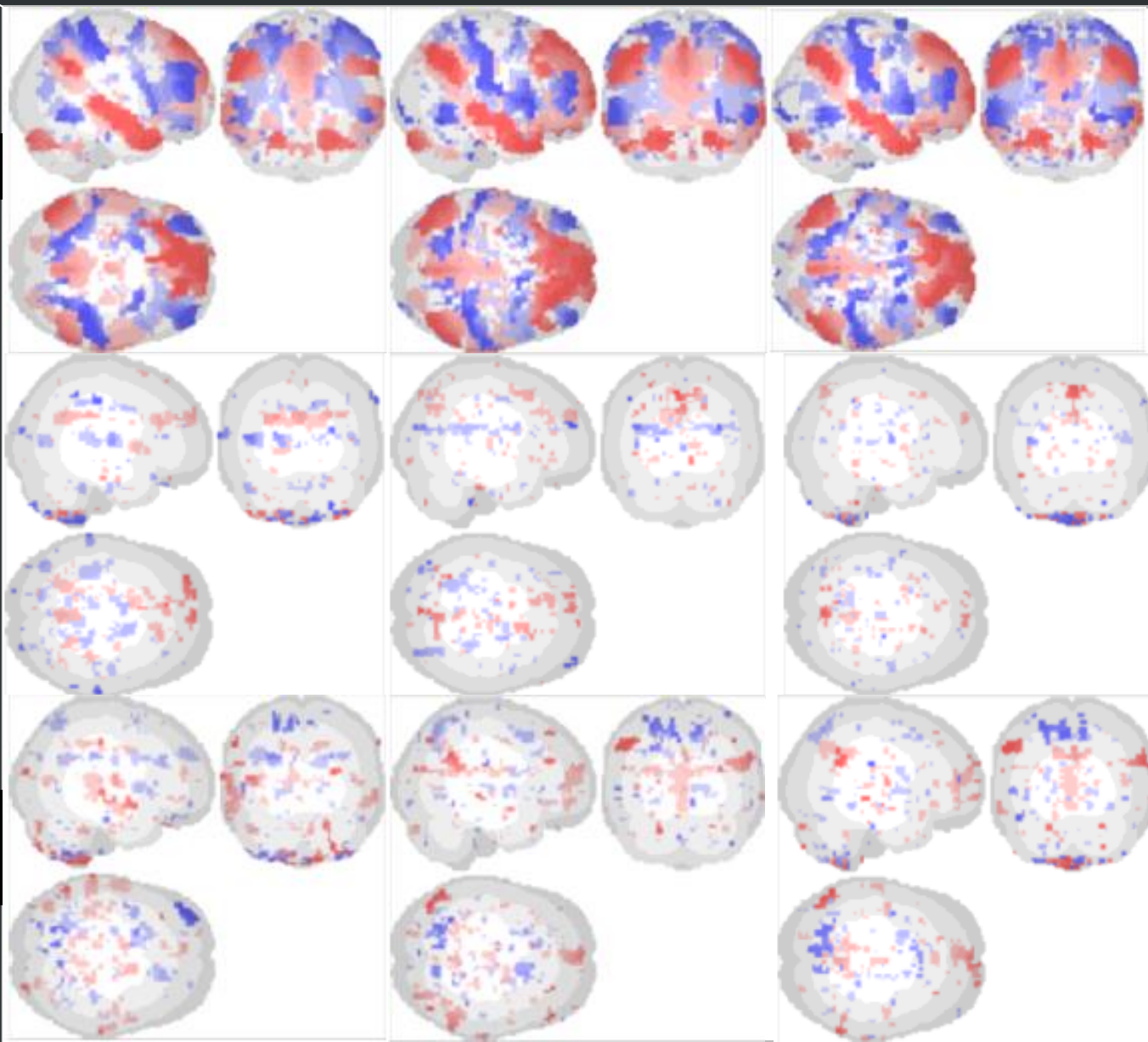
SPM12 OldSeg

SPM12 NewSeg

13

Controls average

Patient average

Contrast
Controls>Patients $p \leq 0.01$
No cluster corr.

fMRI pipelines: propositions

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- **Maintain 2** functional preprocessing **pipelines**:
SPM12 OldSeg & SPM8/VBM
(Alternative: use CONN standardized preprocessing.)
- **Unify into one script** if possible (reproducibility & maintenance, most of the code logic is the same! Only the batch change)
- **Systematic versioning** & centralized repository (petabyte "Softwares" or GitHub):
 - Versioning: ease tracking down original and compare/integrate user changes.
 - Centralized repo: code reviewing (less bugs) and easy update.
- **Validate new pipelines before** deployment: run both current and new pipeline for 1 patient and compare.
- **Freeze** version of **SPM & CONN** (& other necessary softwares) on Z:. Before updating, validate like any new pipeline.

Threshold tweaking

15

- Necessary when only one patient, not enough power



- What is acceptable for clinical?
What is the most plausible?

Threshold tweaking

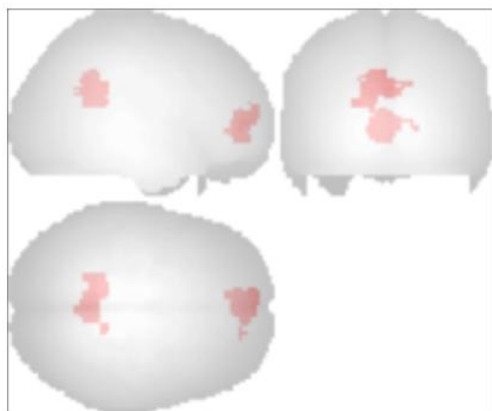
16

Lower height/voxel-wise
threshold

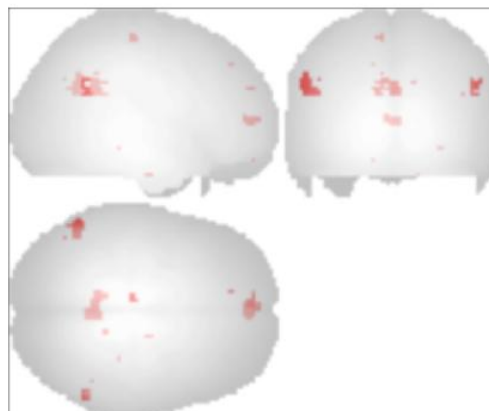
No cluster-wise
correction

Both

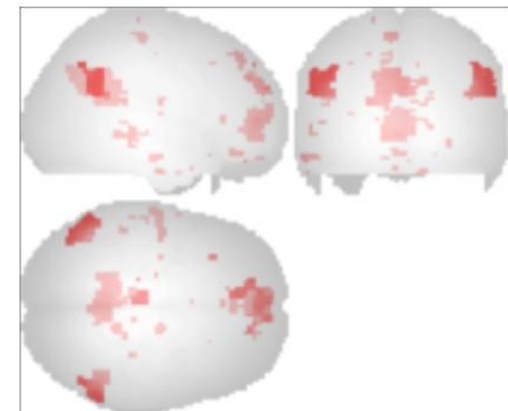
height threshold: $p <$ p-uncorrected
cluster threshold: $p <$ cluster-size p-FWE corrected



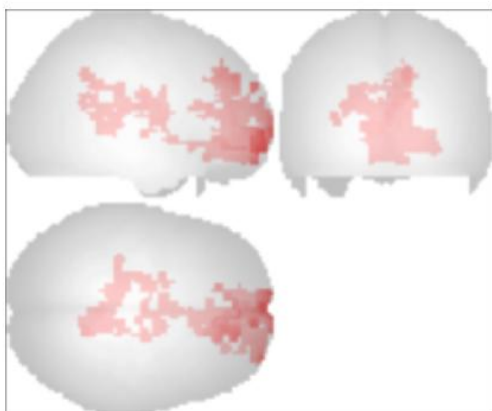
height threshold: $p <$ p-uncorrected
cluster threshold: $k >$ cluster-size



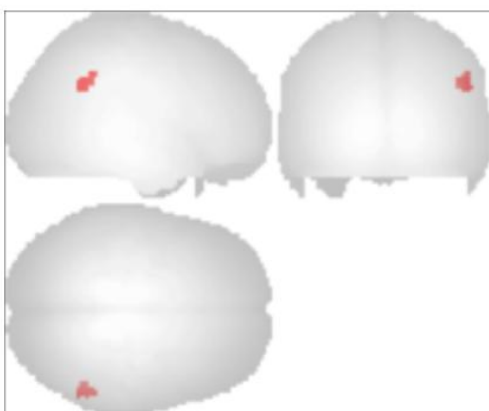
height threshold: $p <$ p-uncorrected
cluster threshold: $k >$ cluster-size



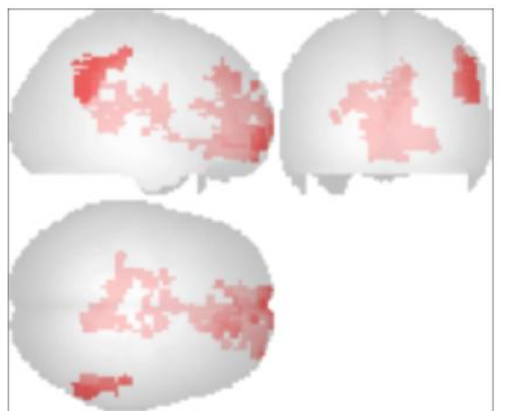
height threshold: $p <$ p-uncorrected
cluster threshold: $p <$ cluster-size p-FWE corrected



height threshold: $p <$ p-uncorrected
cluster threshold: $p <$ cluster-size p-uncorrected



height threshold: $p <$ p-uncorrected
cluster threshold: $p <$ cluster-size p-uncorrected



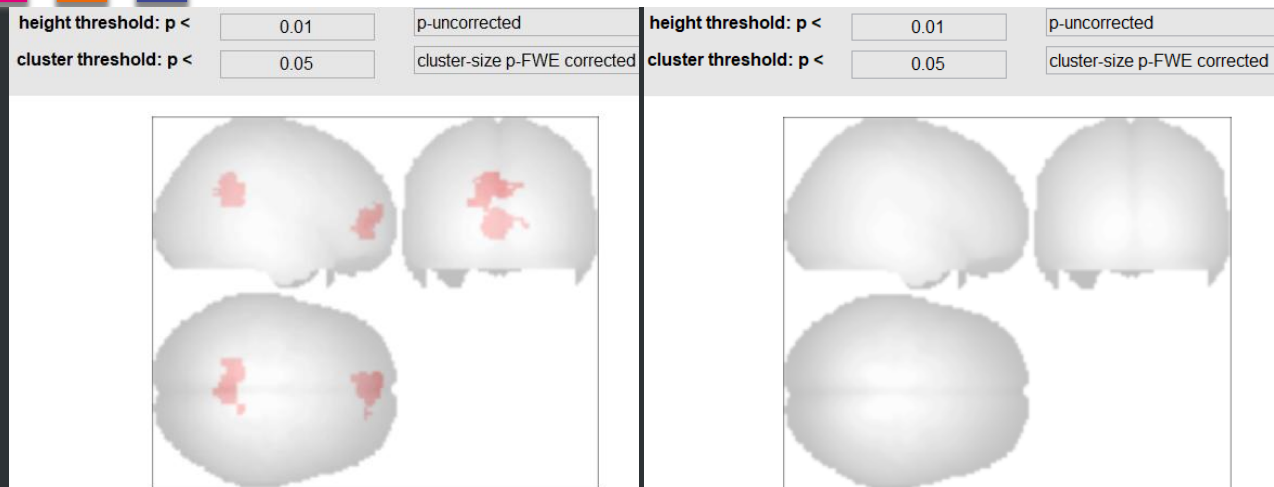
Visualization is not really two-sided

17

Positive

Negative

One-sided



Two-sided



Nothing to show!

Because corrects for
both positive and negative
simultaneously!



Manipulation errors & QA

Control

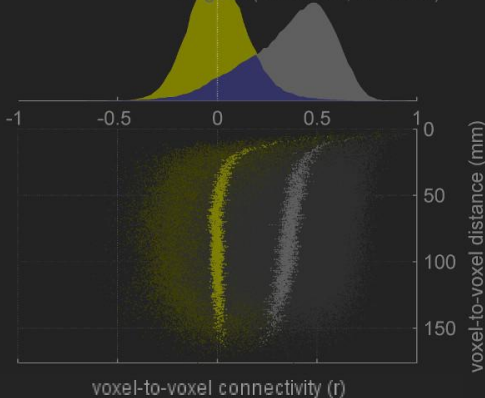
no smooth/realign

Patient

no smooth/realign

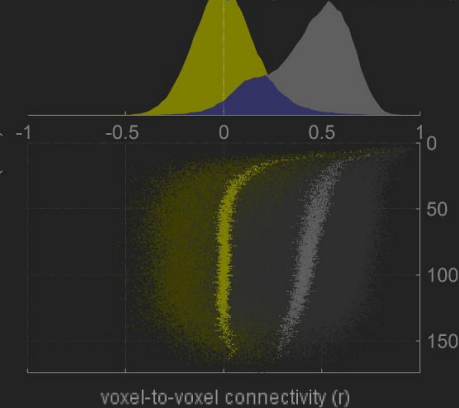
Distribution of connectivity values (r)

after denoising (0.01 ± 0.15 ; $df=87.6$)
original (0.36 ± 0.21 ; $df=296.0$)

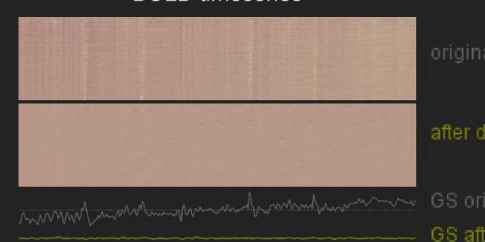


Distribution of connectivity values (r)

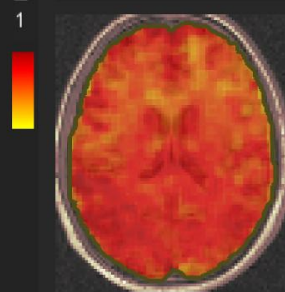
after denoising (0.01 ± 0.17 ; $df=77.1$)
original (0.43 ± 0.20 ; $df=296.0$)



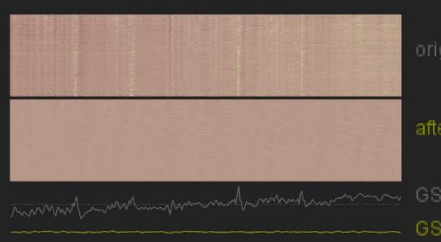
BOLD timeseries



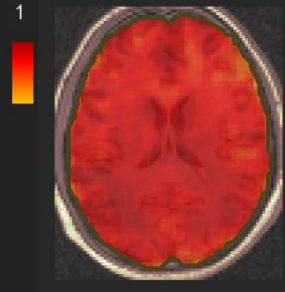
BOLD % variance explained by
TOTAL



BOLD timeseries

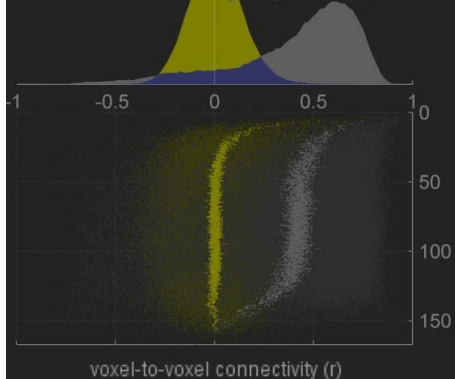


BOLD % variance explained by
TOTAL



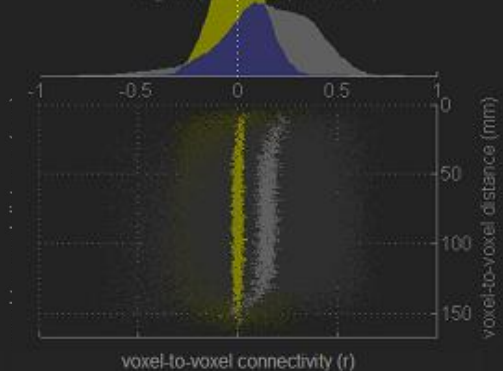
Distribution of connectivity values (r)

after denoising (0.01 ± 0.14 ; $df=86.3$)
original (0.41 ± 0.31 ; $df=296.0$)

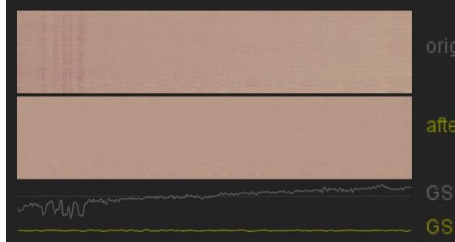


Distribution of connectivity values (r)

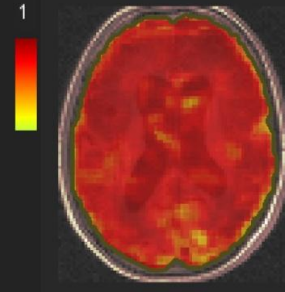
after denoising (0.00 ± 0.12 ; $df=65.9$)
original (0.35 ± 0.23 ; $df=296.0$)



BOLD timeseries



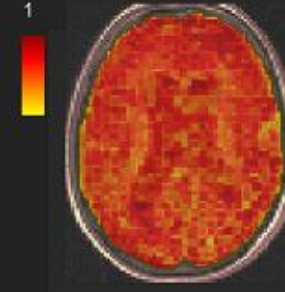
BOLD % variance explained by
TOTAL



BOLD timeseries



BOLD % variance explained by
TOTAL





Manipulation errors & QA

Cause of noisy signal shape!

Control

no smooth/realign

Patient

no smooth/realign

Distribution of connectivity values (r)

Distribution of connectivity values (r)

Distribution of connectivity values (r)

Distribution of connectivity values (r)

after denoising (0.01 ± 0.15 ; $df=87.6$)

after denoising (0.01 ± 0.17 ; $df=77.1$)

after denoising (0.01 ± 0.14 ; $df=86.3$)

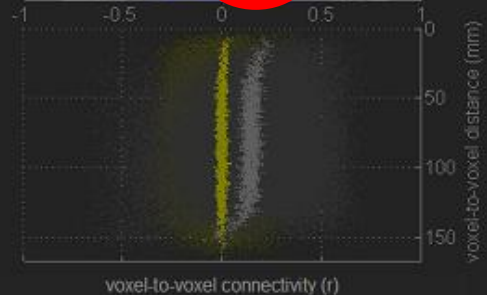
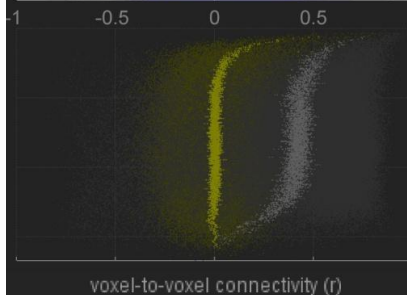
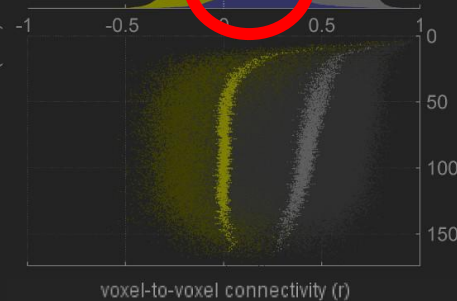
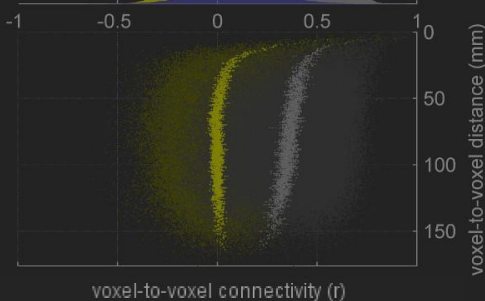
after denoising (0.00 ± 0.12 ; $df=65.9$)

original (0.36 ± 0.21 ; $df=296.0$)

original (0.43 ± 0.20 ; $df=296.0$)

original (0.41 ± 0.31 ; $df=296.0$)

original (0.23 ± 0.23 ; $df=296.0$)



BOLD timeseries

BOLD timeseries

BOLD timeseries

BOLD timeseries

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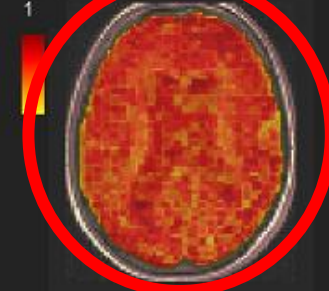
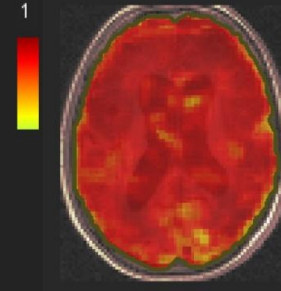
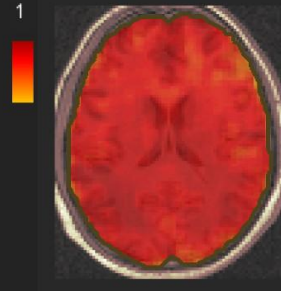
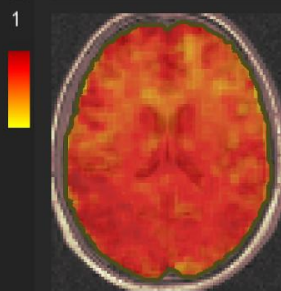
GS aft

BOLD % variance explained by
TOTAL

BOLD % variance explained by
TOTAL

BOLD % variance explained by
TOTAL

BOLD % variance explained by
TOTAL



Other considerations

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- ❑ **Mixed controls**: controls were not reprocessed (different normalization, smoothing kernel, modules versions, resizing, etc.)
- ❑ **Template is CRITICAL**: if bad template, the results will be totally wrong! (Use CONN overlay on MNI to QA)
- ❑ **NaN are CRITICAL**: if you include multiple patients in one CONN project, don't just set to 0, else all patients/subjects are used, including the ones you are trying to exclude! Thus artificially inflating effect size significantly! Inputting NaN instead of 0 will exclude subjects.
- ❑ Lizette mentioned that they did not use VBM/DARTEL at the time to « be able to trust the classifier » ?
- ❑ Interesting: If wrong TR and slice order (slice timing correction), MPFC seed lost all correlation, but not PCC (no change after correction).
- ❑ Ask Mohamed: why in new VBM8 script, coregister on original structural, instead of VBM bias corrected?

Propositions

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- **Automate CONN** project creation: use conn subjects loader script to minimize manip errors
- **Always check Denoising** step for **very weird** artifacts
- **Reprocess controls everytime** we use a new pipeline (else not comparable! eg, normalization different, smoothing kernel can be bigger, etc.)
- Always **write threshold** used in report (voxel p and cluster p)
- For research: **save copy of scripts used on Z:** after study finished (to know version, parameters, modules used, etc.)
- Should always use cerebellum masking?

Conclusion

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- **All pipelines are good**, it is just **difficult** to **migrate** (and to learn how to use them)
- One **very stable** pipeline, used for years (SPM12 OldSeg/Athena's). Should use that!
- **Version, centralize, unify & fix code** potentially useful to reduce errors or be more descriptive (parameters for easy **migration**, conn subjects loader, fix bugs or message)
(also it will be faster for users 😊)
→ updated SPM12 OldSeg already done, eventually merged with Mohamed's code on GitHub? 😊
- **VBM** should be kept, but mostly for research (where segmentation matters & more conservative results).
→ Move to **CAT12**? (better report and segmentation more customizable, encouraging first results)

Thank you for your attention

References:

- N/A



James S. McDonnell Foundation



Université de Liège



BONUS SLIDES

