

From voxel to complex network

Data integration in medical imaging

Marco Diego Dominietto

Biomaterials Science Center, University of Basel
Department of Surgery and Orthopedics, Hospitals Schaffhausen, Switzerland

Traitemet d'Images en Physique Médicale

Port-Bourgenay , October 7-9, 2015



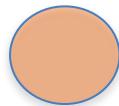
Department of
**Biomedical
Engineering**

spitäler schaffhausen



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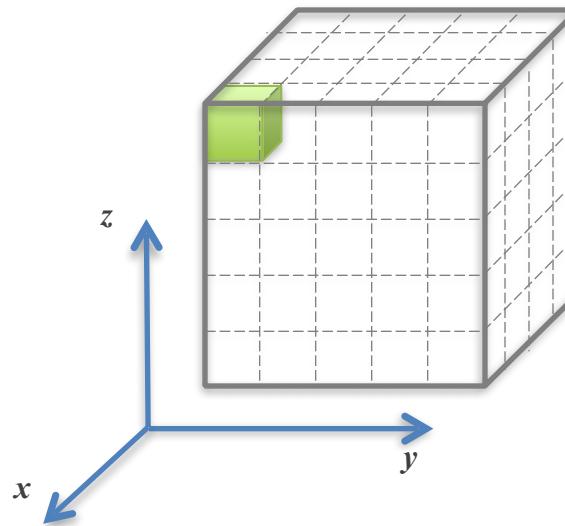


Voxel

Def: In 3D images, a voxel is a unit of graphic information that defines a point in three-dimensional space. For a given image modality, a voxel is the minimum measurable volume.

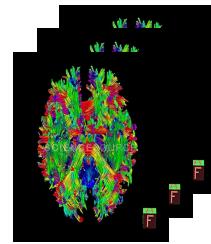
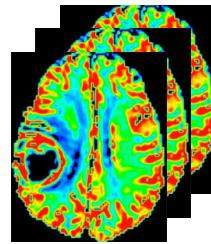
$$v = v(x, y, z)$$

Spatial domain \Re^3

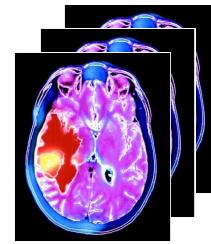


Multi-modalities approach allows to have more information about anatomical details and physiological properties of the same tissue. For each modality we can extract one or more **features**.

- perfusion
- glucose metabolism
- oxygen distribution
- vascular structure
- permeability
- CA uptake
- blood velocity
- etc.

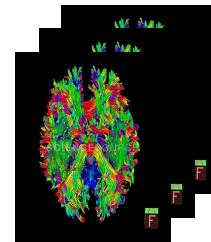
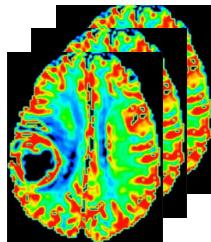
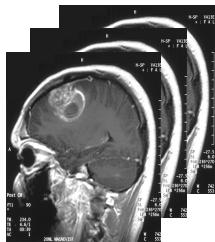


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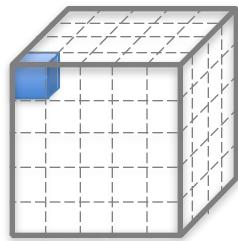
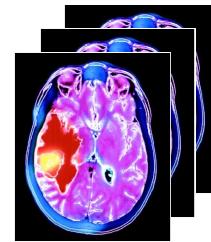


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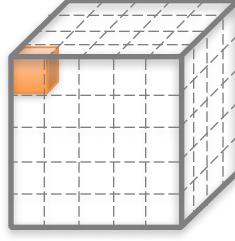


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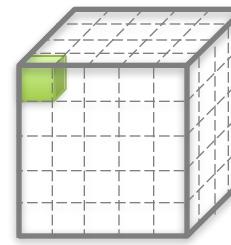


Feature

F_1

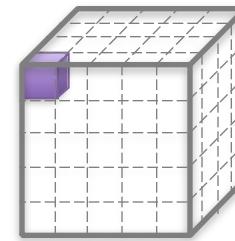


F_2



F_3

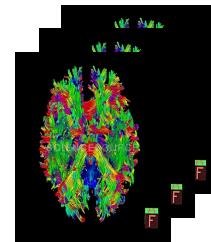
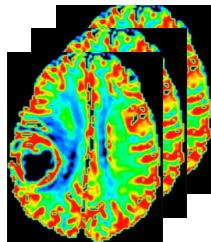
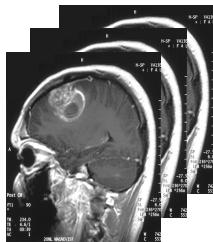
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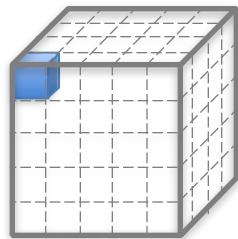
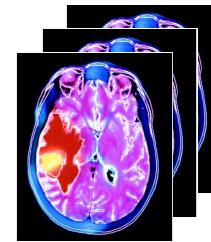
F_N

Multi-modalities approach allows to have more information about anatomical details and physiological properties of the same tissue. For each modality we can extract one or more **features**.

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- permeability
- blood velocity
- glucose metabolism
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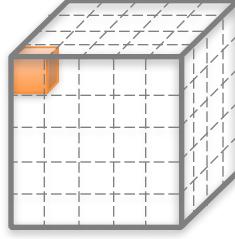


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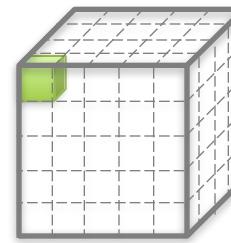


Feature

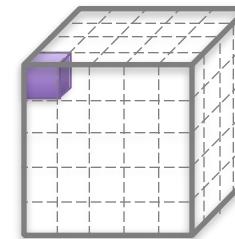
F_1



F_2



F_3



F_N

$$v = v(x, y, z)$$

Spatial domain \Re^3

$$v = v(F_1, F_2, F_3, \dots, F_N)$$

Features domain \Re^N

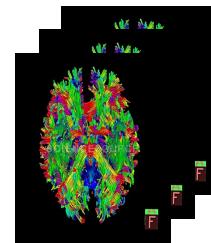
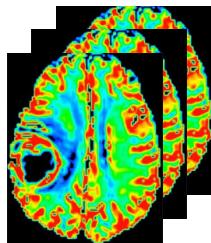
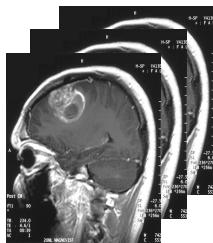
$$v = v(F_1(t), F_2(t), F_3(t), \dots, F_N(t))$$

Time domain

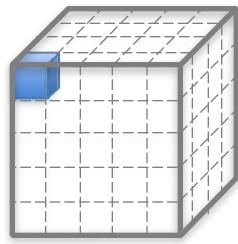
$$\Re^1$$

Multi-modalities approach allows to have more information about anatomical details and physiological properties of the same tissue. For each modality we can extract one or more **features**.

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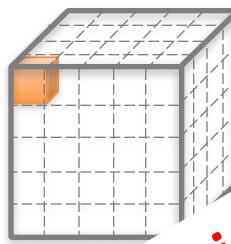


.....



Feature

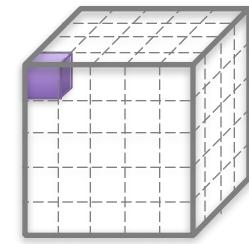
F_1



a lot of information !



F_3



F_N

$$v = v(x, y, z)$$

Spatial domain \Re^3

$$v = v(F_1, F_2, F_3, \dots, F_N)$$

Features domain \Re^N

$$v = v(F_1(t), F_2(t), F_3(t), \dots, F_N(t))$$

Time domain \Re^1

How to keep into account all these information?

...it isn't a co-registration problem!

Data Integration

complexity

Spatial domain \Re^3

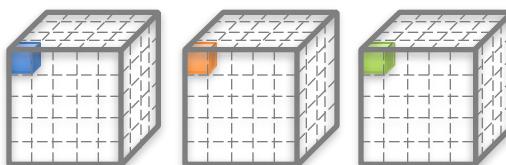
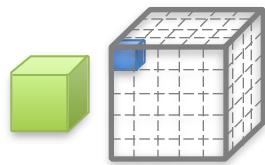
Spatial domain \Re^3

Features domain \Re^N

Spatial domain \Re^3

Features domain \Re^N

Time domain \Re^1



Shape analysis

Texture analysis

Complex Network

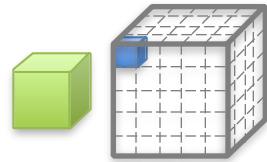
Pattern recognition

Clustering

Data Integration

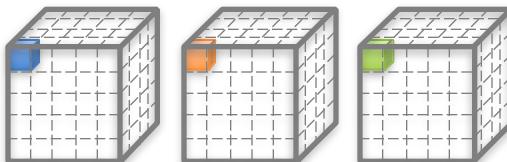
complexity

Spatial domain \Re^3



Spatial domain \Re^3

Features domain \Re^N



Spatial domain \Re^3

Features domain \Re^N

Time domain \Re^1



Shape analysis

Texture analysis

Complex Network

Pattern recognition

Clustering

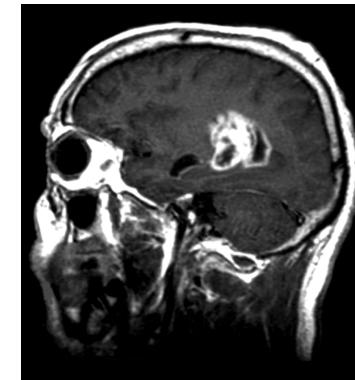
What is our goal?

The diagnosis of a suspected lesion faces two basic problems:

- 1 **detection** of the suspected lesion



healthy brain

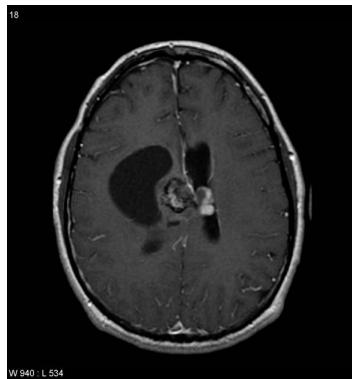


glioma

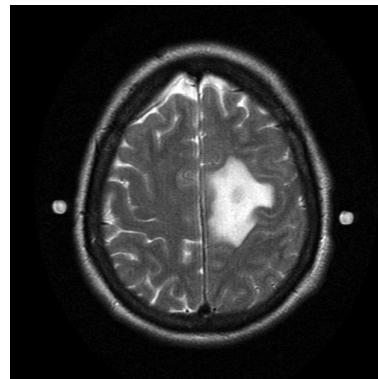
disease

yes no

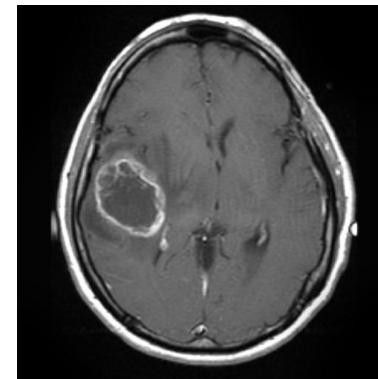
- 2 **classification** of the lesion



Pilocytic astrocytoma



anaplastic astrocytoma



glioblastoma multiforme

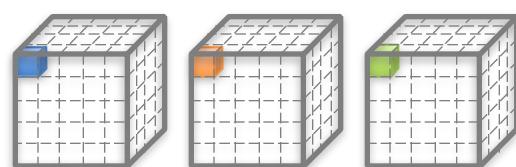
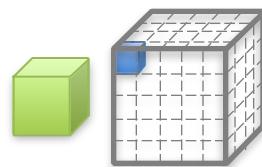
disease

grade

Data Integration

Spatial domain \Re^3

Features domain \Re^N



Shape analysis

perimeter

volume

surface area

compactness

Texture analysis

histogram

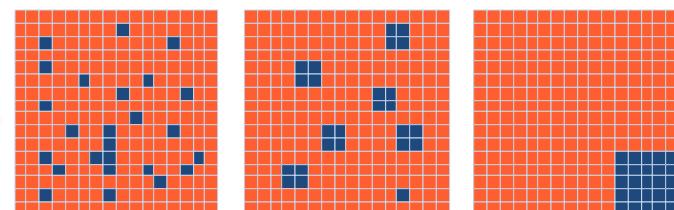
fractal dimension

lacunarity

Fourier transf.



6 moments of the normal distribution:
mean, st.dev., etc.



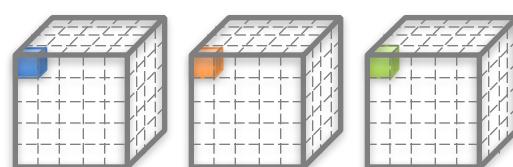
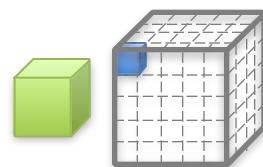
Same number of lacunas (25) but three different values of Λ ($\Lambda_1 > \Lambda_2 > \Lambda_3$)

Data Integration

Spatial domain \Re^3

Spatial domain \Re^3

Features domain \Re^N



Shape analysis

perimeter

volume

surface area

compactness

Texture analysis

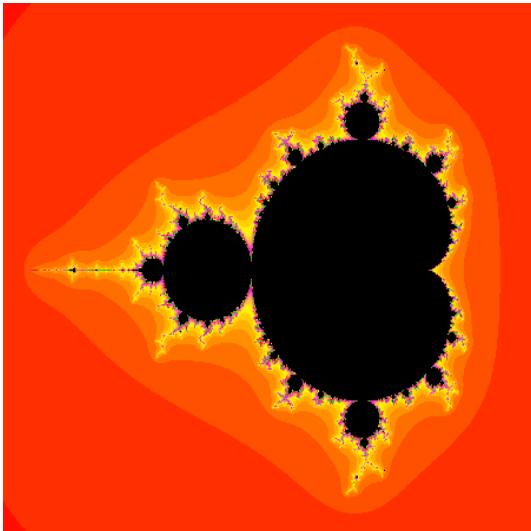
histogram

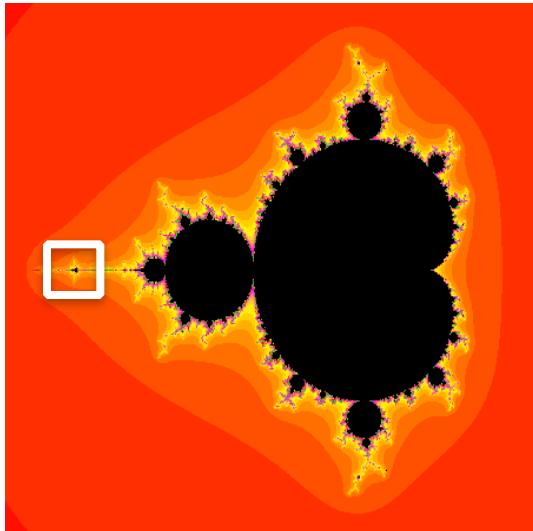
fractal dimension

lacunarity

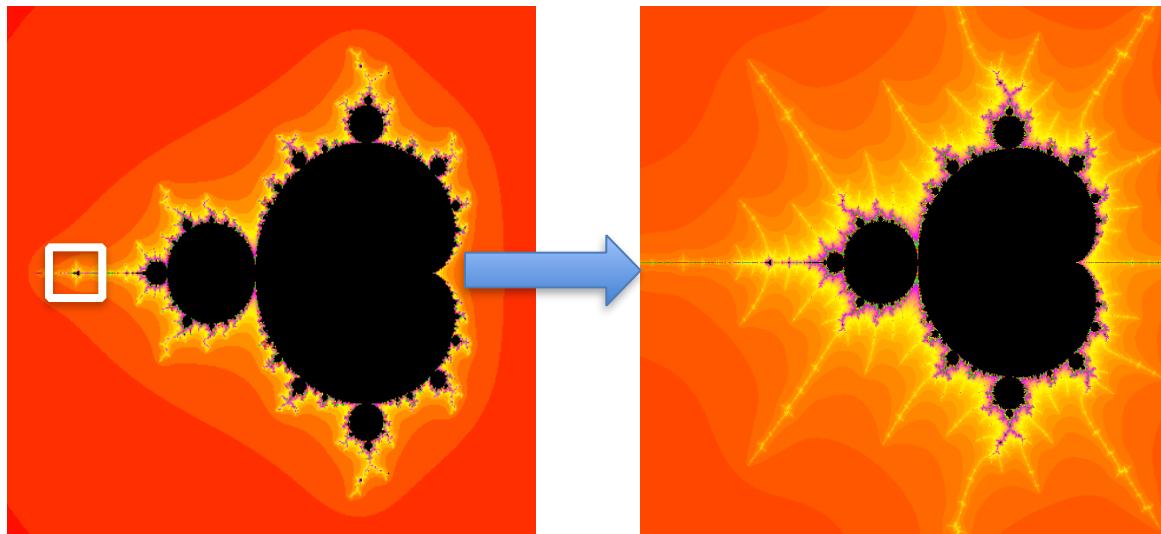
Fourier transf.

Fractal Dimension

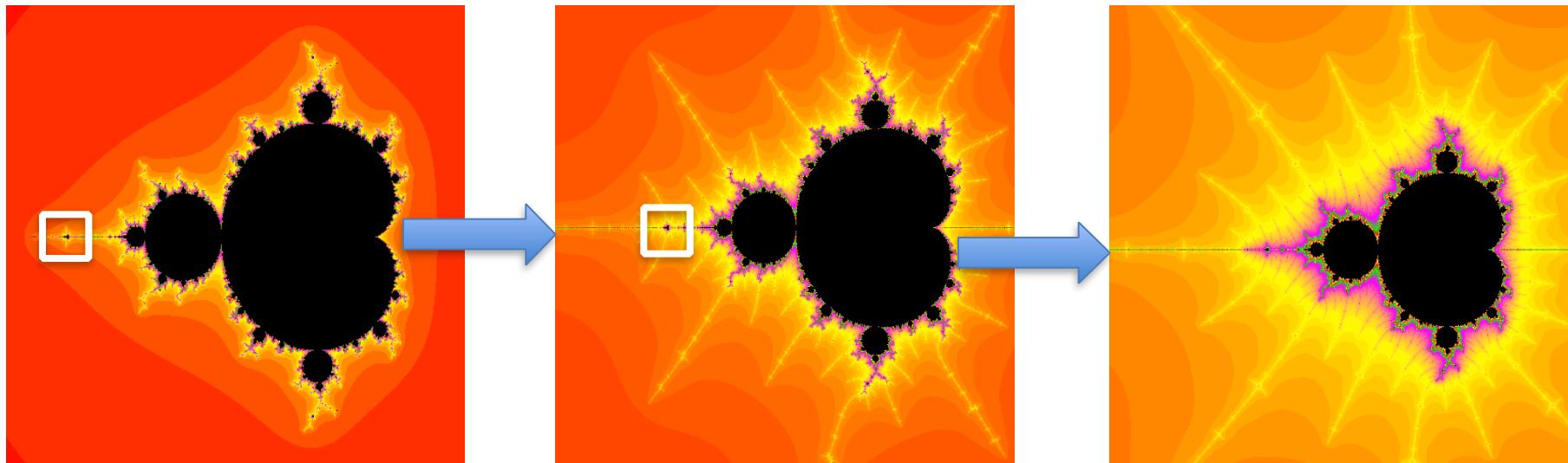




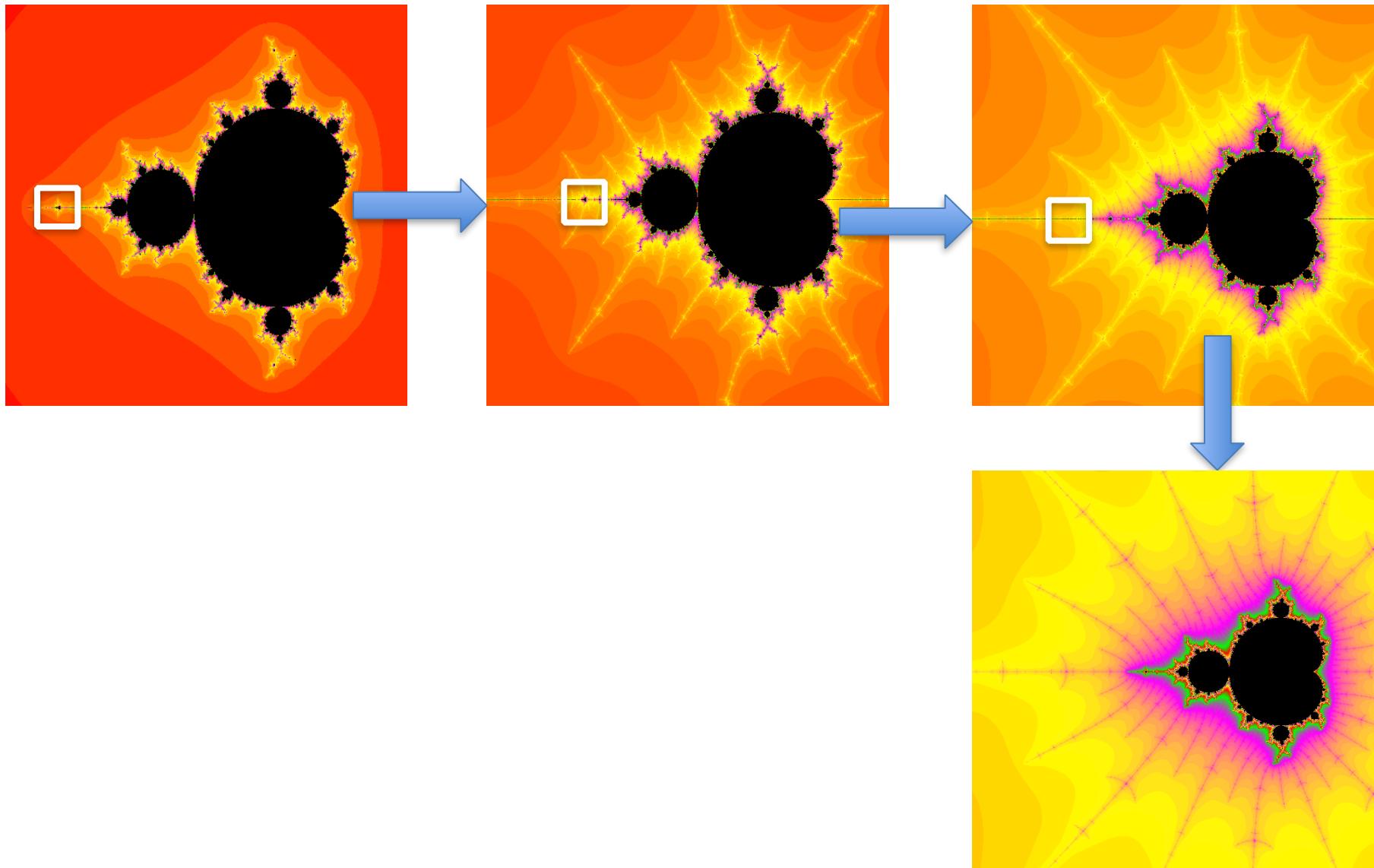
Fractal Dimension



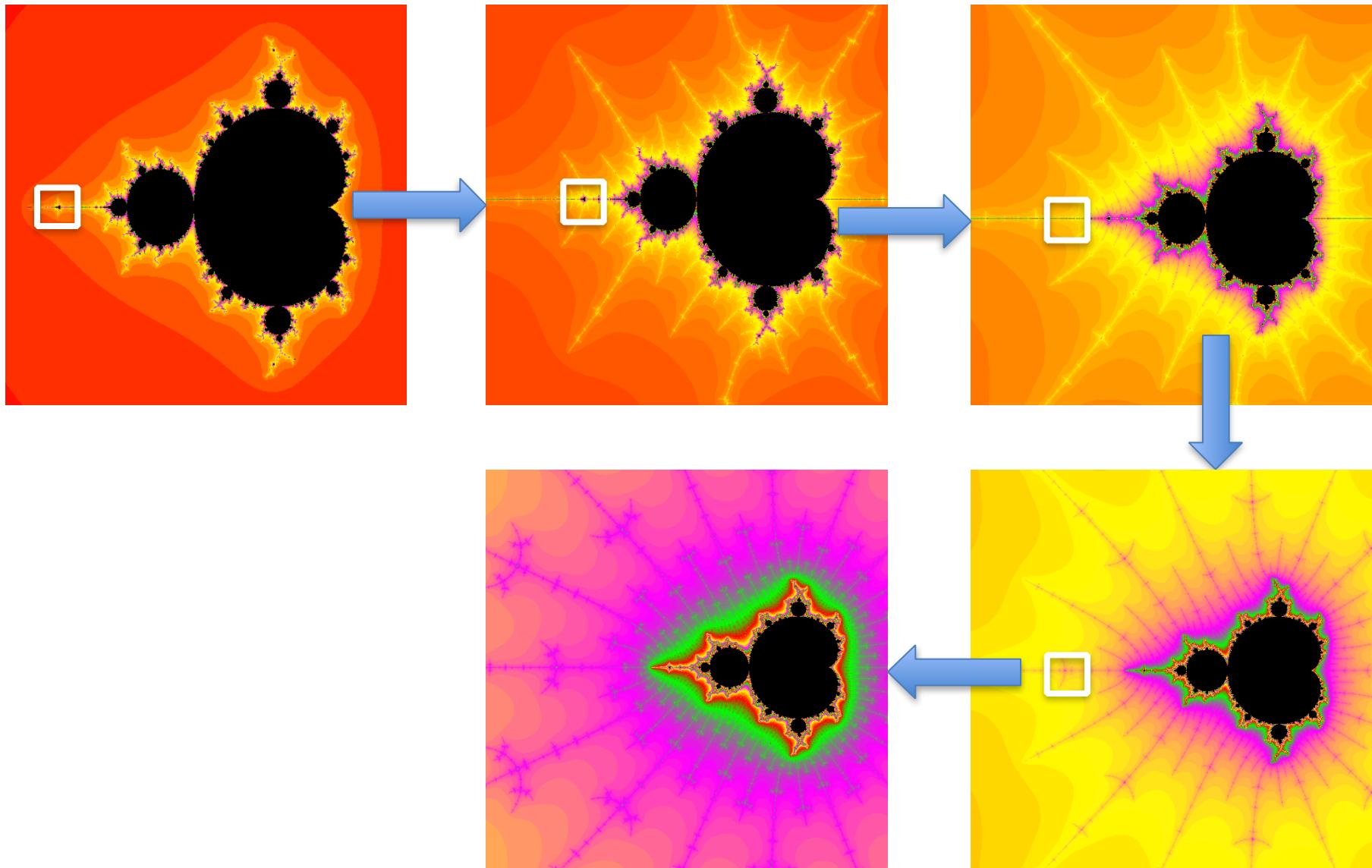
Fractal Dimension



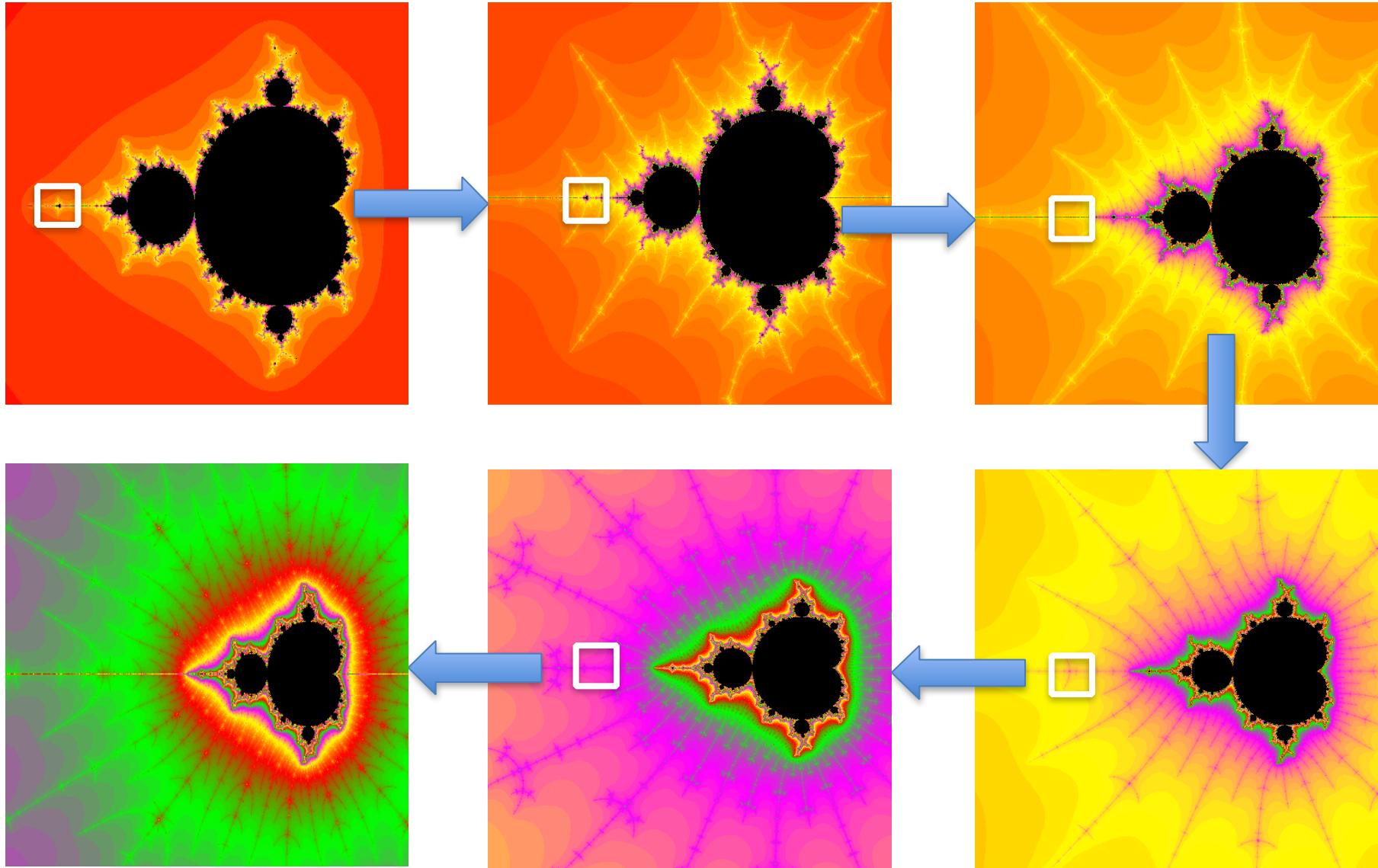
Fractal Dimension



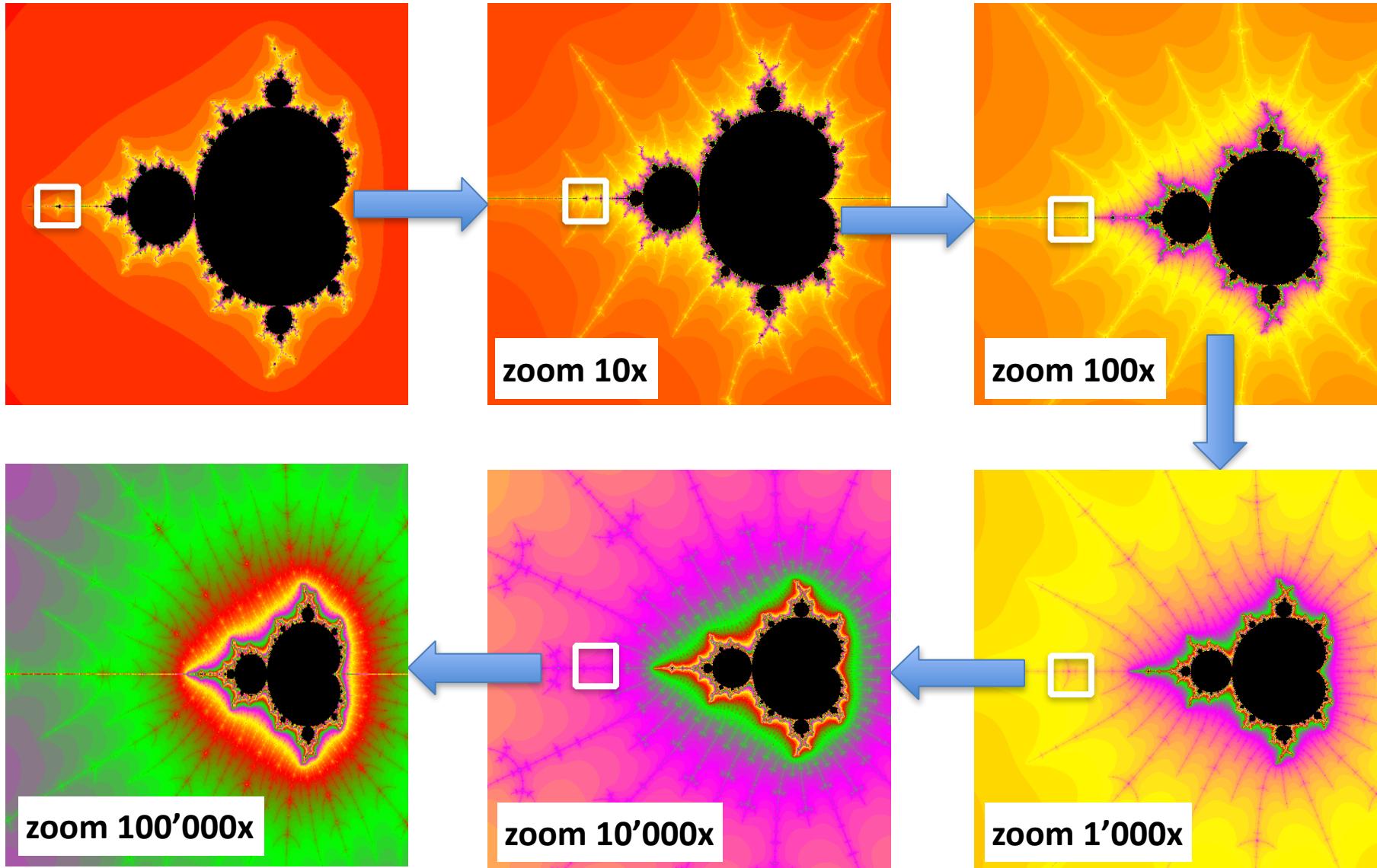
Fractal Dimension

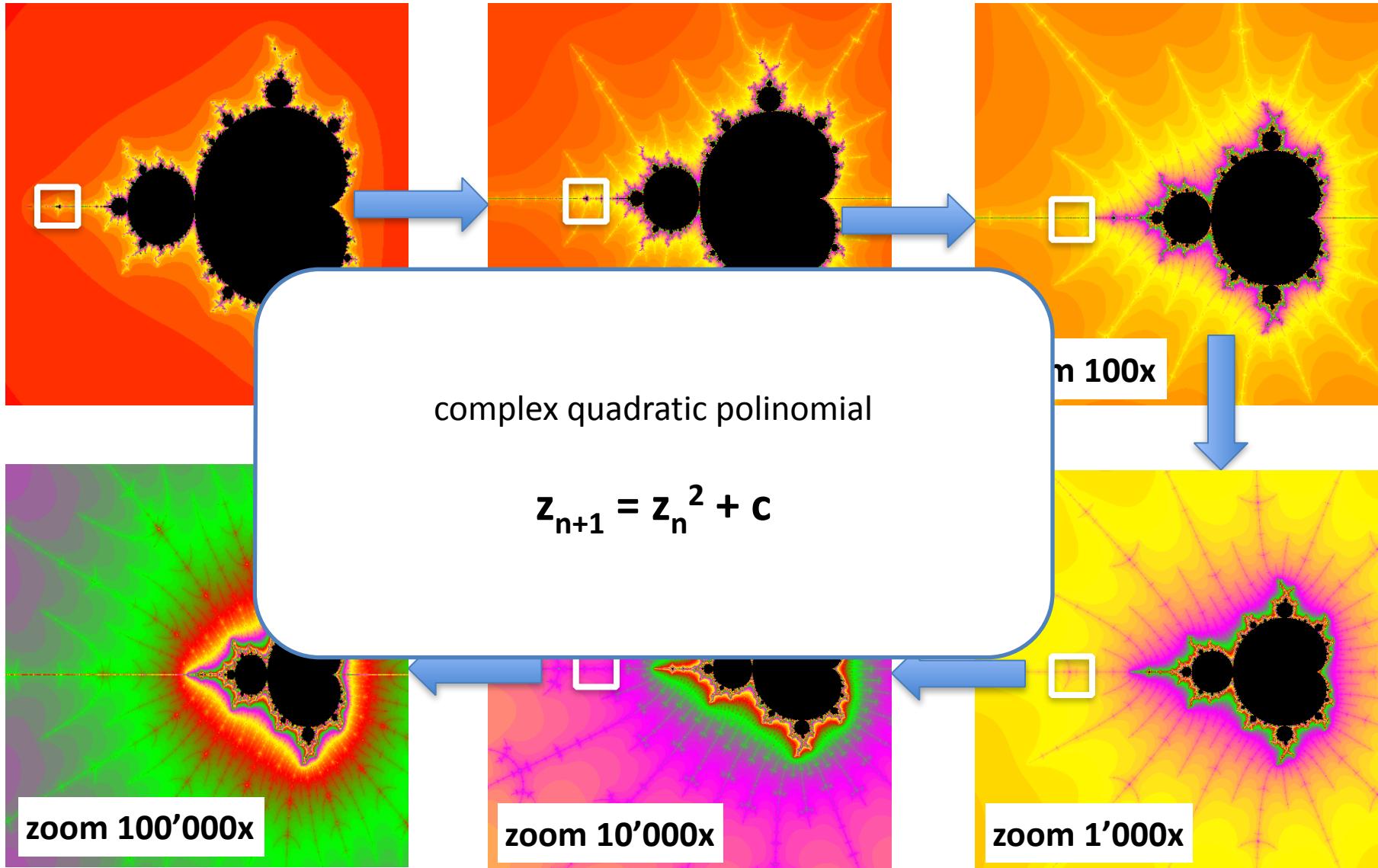


Fractal Dimension

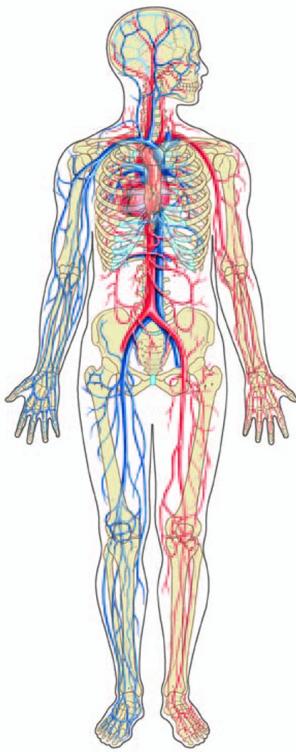


Fractal Dimension





This **self-similar fractal structure** is the optimal model developed by **Nature** to accomplish those tasks

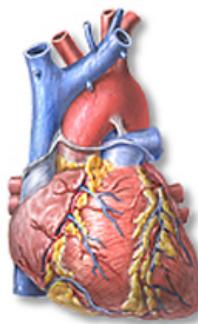
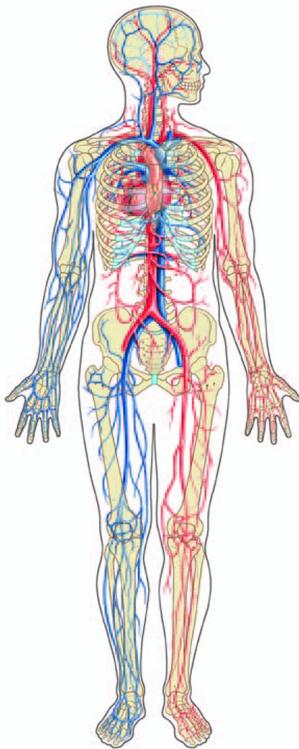


- Distribute the blood to **several organs**
- Delivery **different quantity** of blood
- Transform the blood flow from pulsed to **continuous**
- Remove the **waste** (metabolites, CO₂,...)
- It should **work continuously** for 80 years, longer is better!

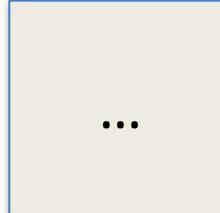
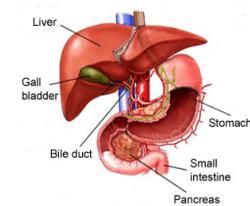
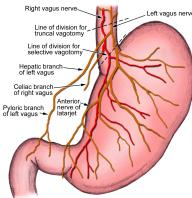
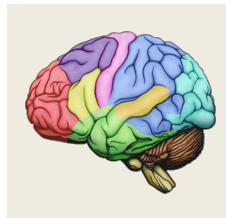
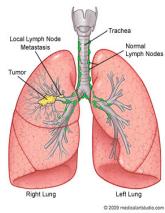
$$D = \lim_{r \rightarrow \infty} \frac{\log N(r)}{-\log \left(\frac{1}{r} \right)}$$

D = dimension
N = number of self similarity (3)
r = reduction factor (2)

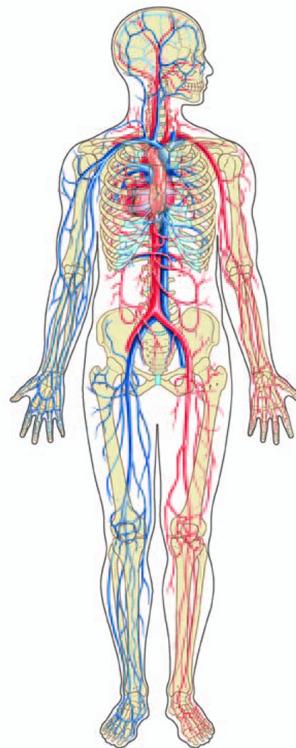
Vascular system



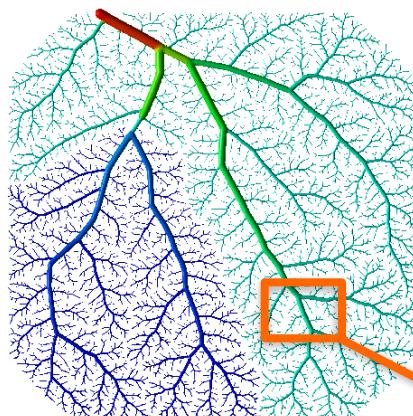
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Vascular system



vessel tree

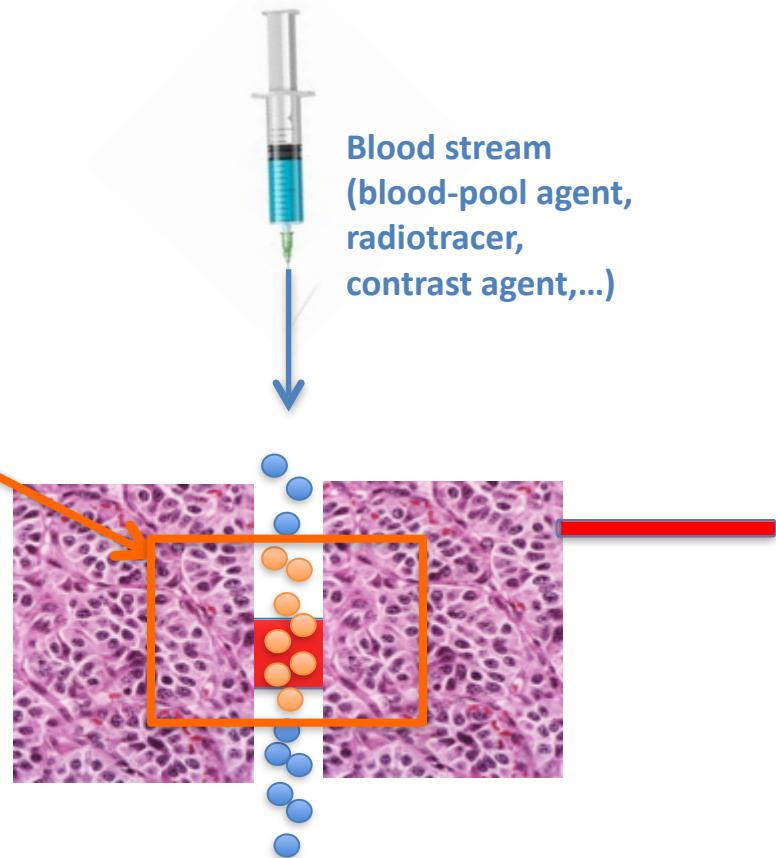


non-permeable healthy vessel

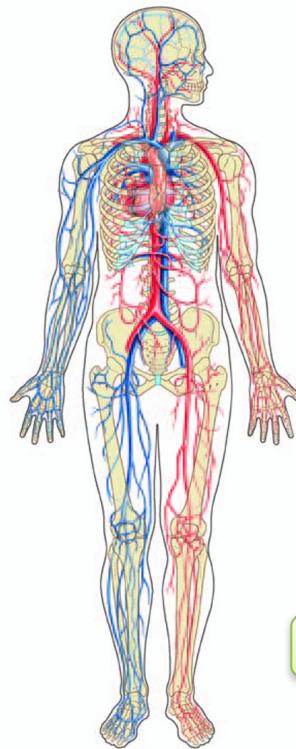
perfusion

BF

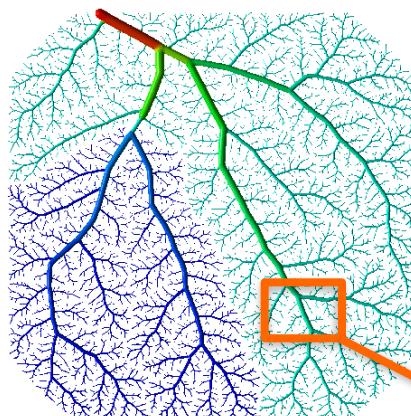
volume of blood in velocity of the
the voxel (BV) blood in the voxel



Vascular system



vessel tree



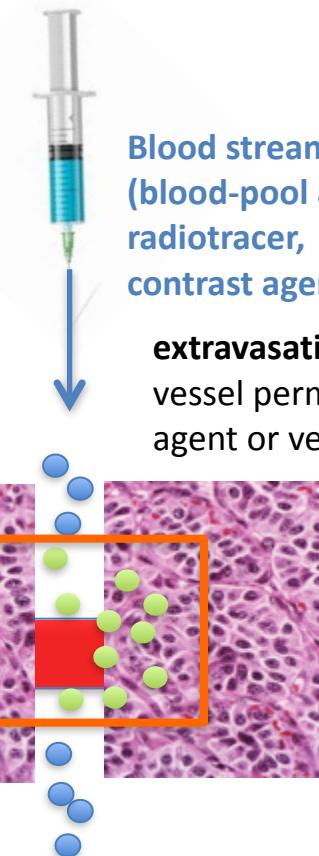
permeable non healthy vessel

permeability

extravasation

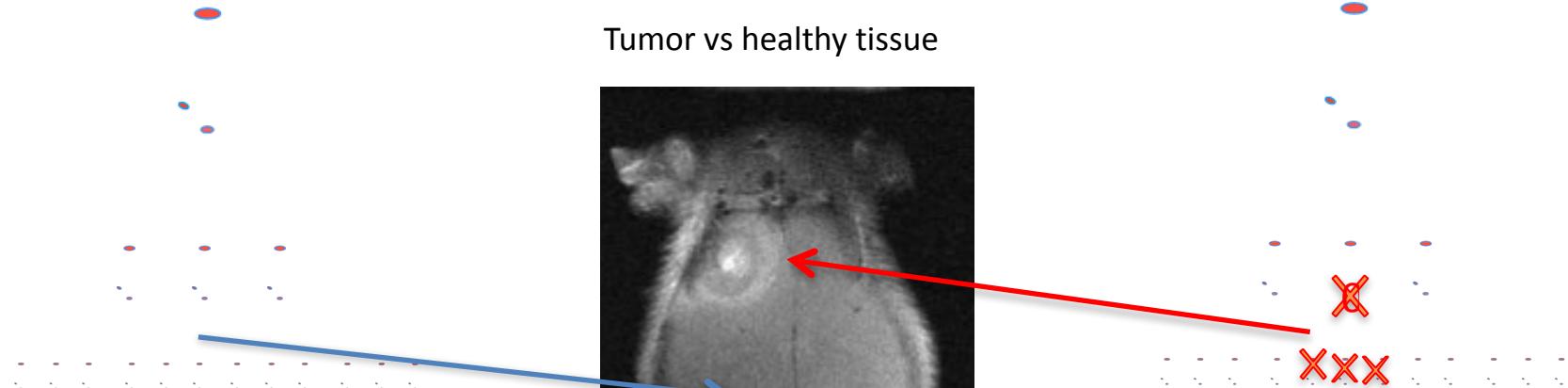
blood transfer constant from
vascular compartment to
extracellular space

volume of blood extravasated into
extracellular space

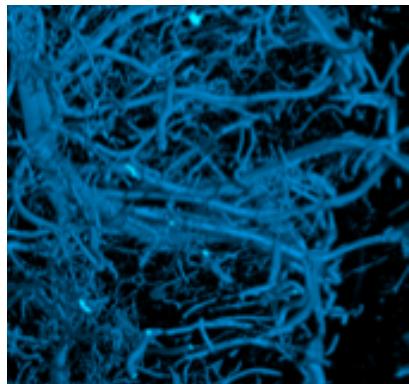
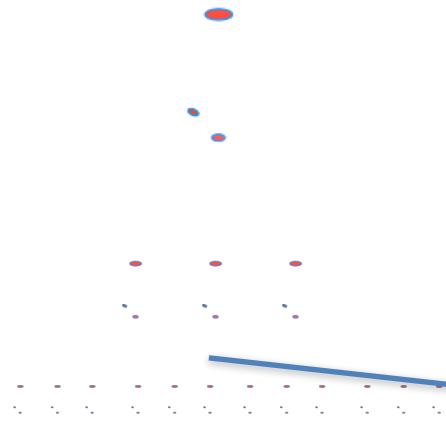


Blood stream
(blood-pool agent,
radiotracer,
contrast agent,...)

extravasation:
vessel permeable to contrast-
agent or vessel damaged (leaky)



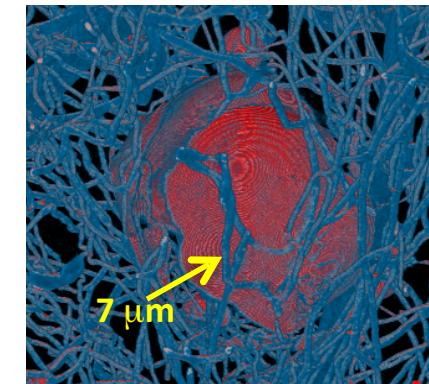
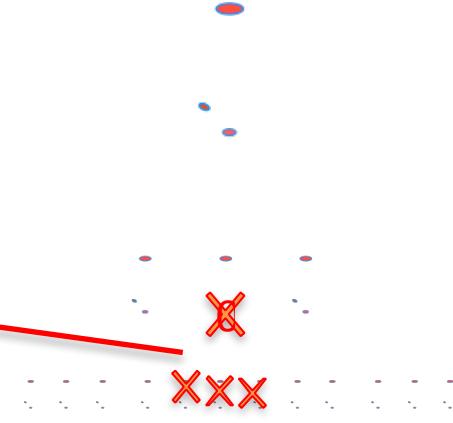
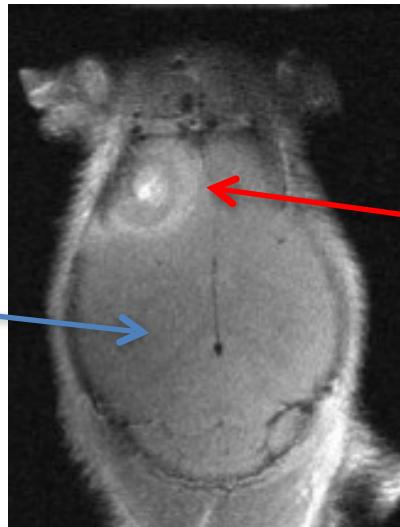
Murine glioma GL261
T1-w MRI – CA: Gd-Dota



More **organized** structure of vessel network
Fractal Dimension = 2.23 ± 0.02

October 8, 2015 – Port-Bourgenay, France

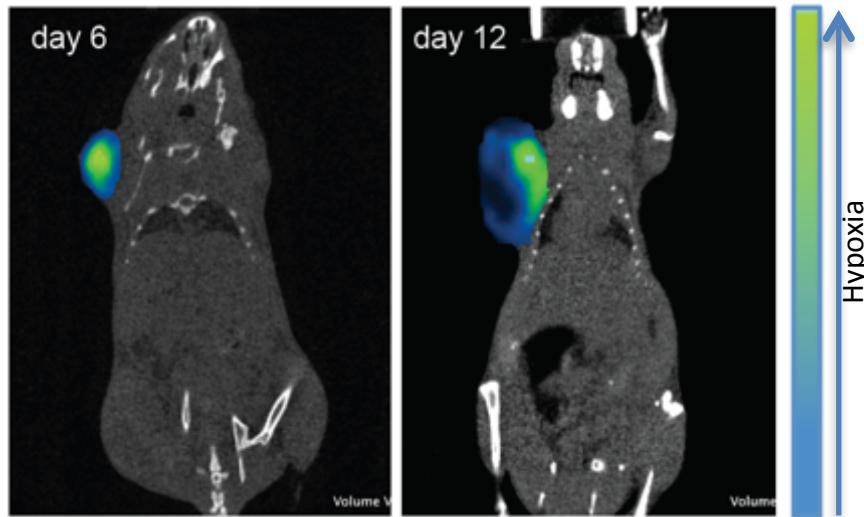
Tumor vs healthy tissue



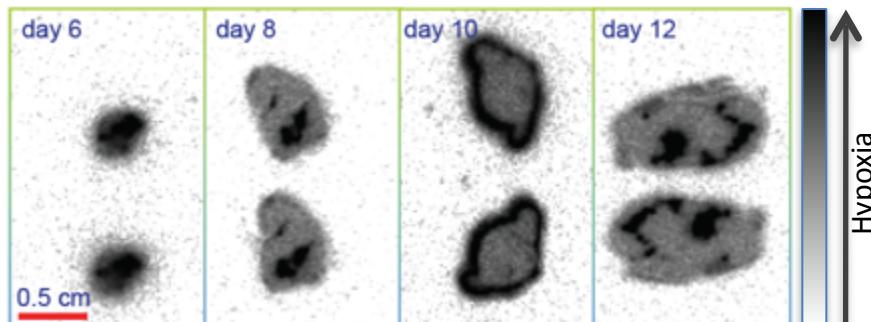
Chaotic structure of vessel network
Fractal Dimension = 2.78 ± 0.03

Marco Dominietto

Hypoxia evaluation



18F-MISO PET/CT C51 murine tumor



Autoradiography

Hypoxia

Hypoxia level is a **trigger** of the angiogenesis

18F-MISO diffuse into the cells:

- **aerobic condition:** the radical compound is reoxidized and diffuse out of the cells
- **hypoxic condition:** it is bind to intracellular macro-molecules and accumulate inside the cell.

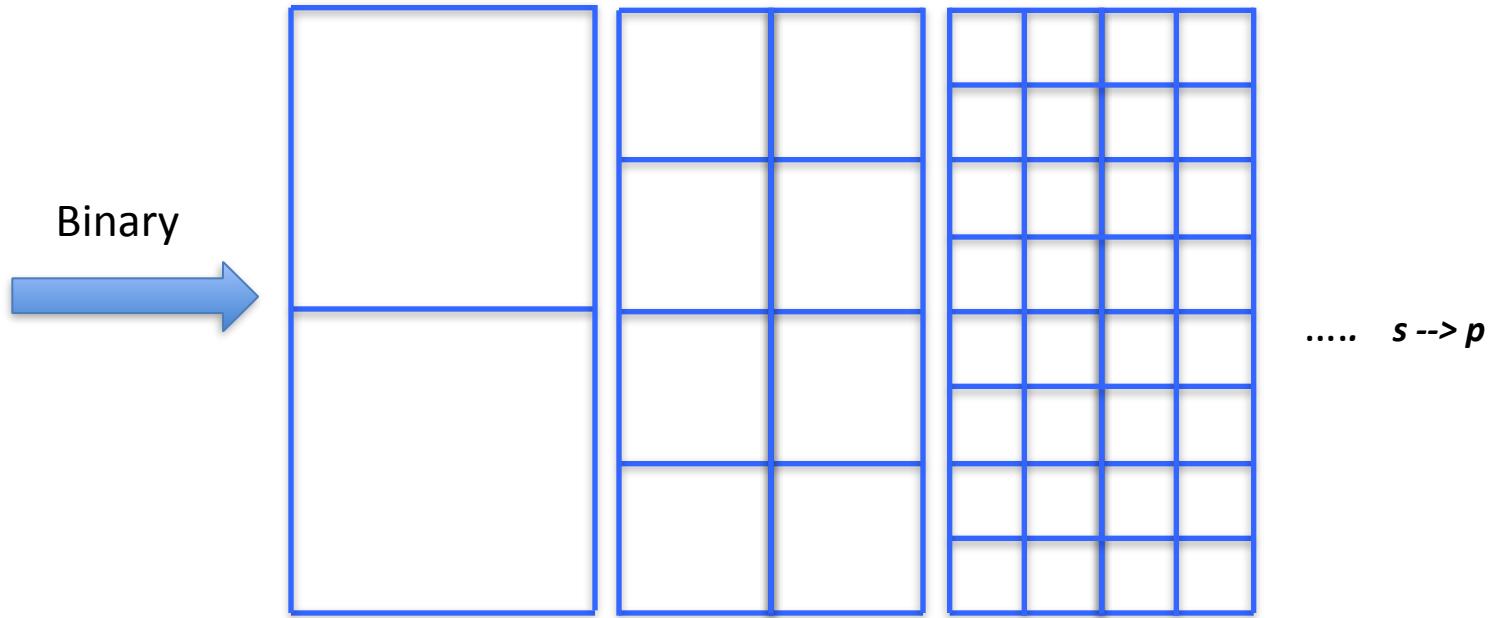
Heterogeneous distribution of ¹⁸F-MISO during tumor growth

Collaboration with: Steffi Lehmann (IBT, ETHZ), Michael Höner (AIC-PET, ETHZ)

October 8, 2015 – Port-Bourgenay, France

Marco Dominietto

Box Counting - BC



FD = Fractal Dimension

$N(s)$ = number of box needed to cover the image

s = size of the box

p = pixel dimension

$$D = \lim_{s \rightarrow p} \frac{\log N(s)}{-\log(s)}$$

Russel, D., Hanson, J., Ott, E., 1980. *Dimension of strange attractors*. Physical Review Letters 45 (14), 1175–1178

Benoit B. Mandelbrot , *The Fractal Geometry of Nature*, Spektrum Akademischer Verlag; 1990

Data Integration

complexity

Spatial domain

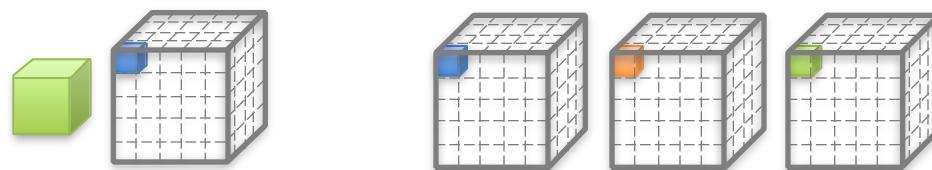
\Re^3

Spatial domain

\Re^3

Features domain

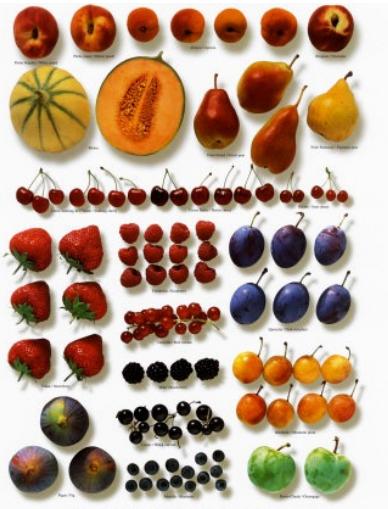
\Re^N



Shape analysis

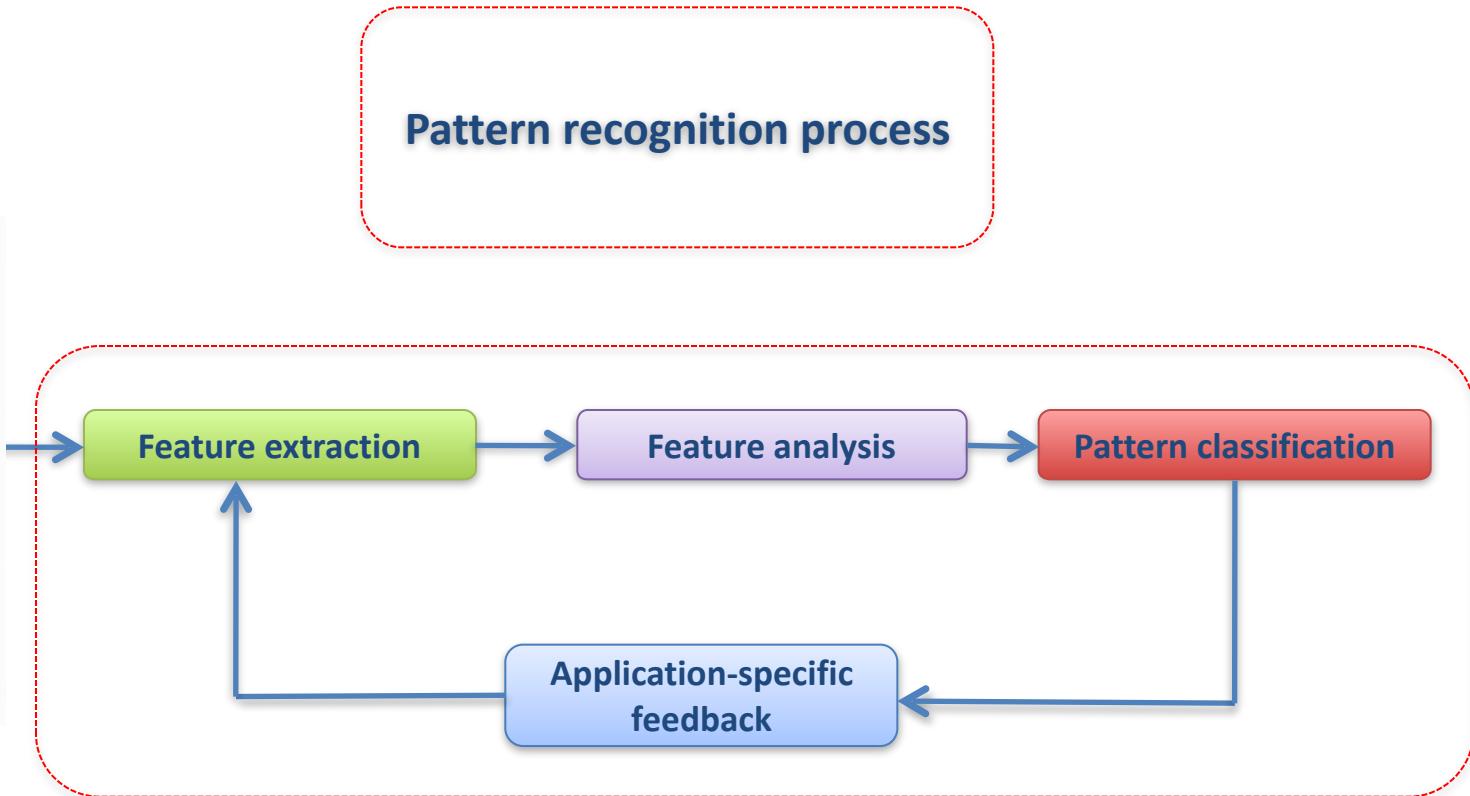
Texture analysis

Pattern recognition



Black BOX

	peach		prune
	melon		apple
	sliced melon		cassis
	pear		strawberry
	fig		raspberry
	apricot		blueberry
	cherries		blackberry
	red currant		



Feature extraction

Goal 1: individuate the objects **inside** the image



Shape analysis

Original image



$D(x,y,z)$

Objects: A, B,N

Feature extraction

Goal 1: individuate the objects **inside** the image

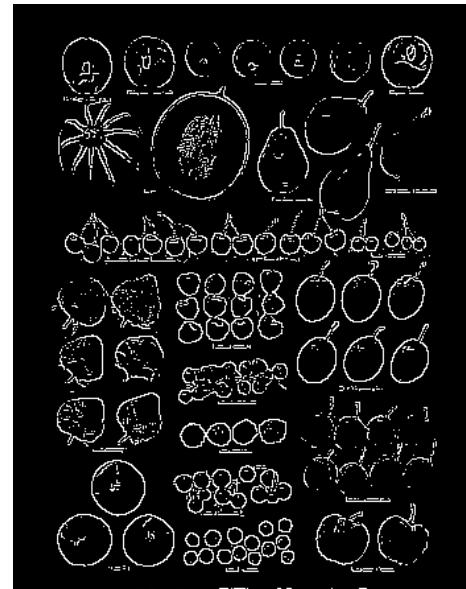
Shape analysis

Original image



$D(x,y,z)$

Contours



$C(x,y,z)$

Mask

$M(x,y,z)$

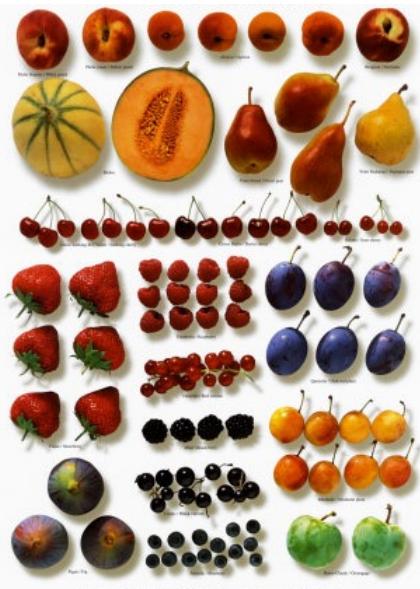
Objects: A, B,N

Feature extraction

Goal 1: individuate the objects **inside** the image

Shape analysis

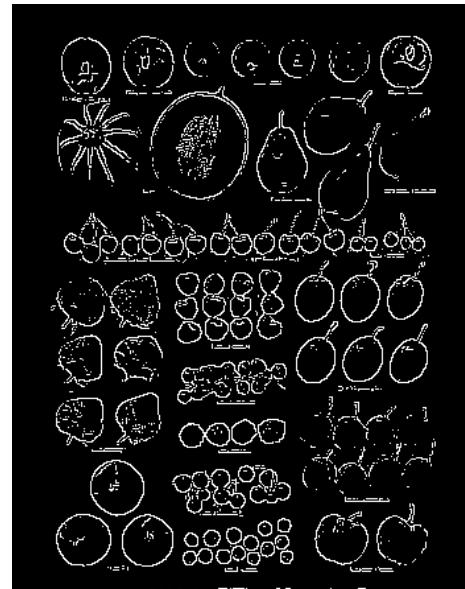
Original image



Feature extraction
operators

F_C, F_M, \dots

Contours



$D(x,y,z)$

$C(x,y,z)$

$M(x,y,z)$

Contour = $F_C(D)$

Mask = $F_M(D)$

Objects: A, B,N

Feature analysis

Goal 2: evaluate **morphological parameters** of each extracted objects (A, B ,..N)

SHAPE

perimeter

volume

surface area

compactness

....



Objects with different shapes.

TEXTURE

histogram

fractal dimension

lacunarity

Fourier transf.

....



Objects with similar shapes but different texture

morphological parameters matrix

$$\mathbf{A}(S_A, V_A, C_A, (m_1 m_2 \dots m_6)_A, FD_A, \Lambda_A, \dots)$$

$$\mathbf{B}(S_B, V_B, C_B, (m_1 m_2 \dots m_6)_B, FD_B, \Lambda_B, \dots)$$

...

$$\mathbf{N}(S_n, V_n, C_n, (m_1 m_2 \dots m_6)_n, FD_n, \Lambda_n, \dots)$$



feature space IR^n

n = number of evaluated features

Pattern classification

Goal 3: automatically classify the extracted objects on the basis of their features information.

At this level we have extracted those objects in the features space. At this stage we can **only say that the object are different.**

surface		S_A		S_B	\dots	N	S_n
volume		V_A		V_B			V_n
compactness		C_A		C_B			C_n
histogram moments		$(m_1 \ m_2 \ \dots \ m_6)_A$		$(m_1 \ m_2 \ \dots \ m_6)_B$			$(m_1 \ m_2 \ \dots \ m_6)_n$
fractal dimension		FD_A		FD_B			FD_n
lacunarity		Λ_A		Λ_B			Λ_n
....							

Clustering measures

Distance measures

Similarity measures

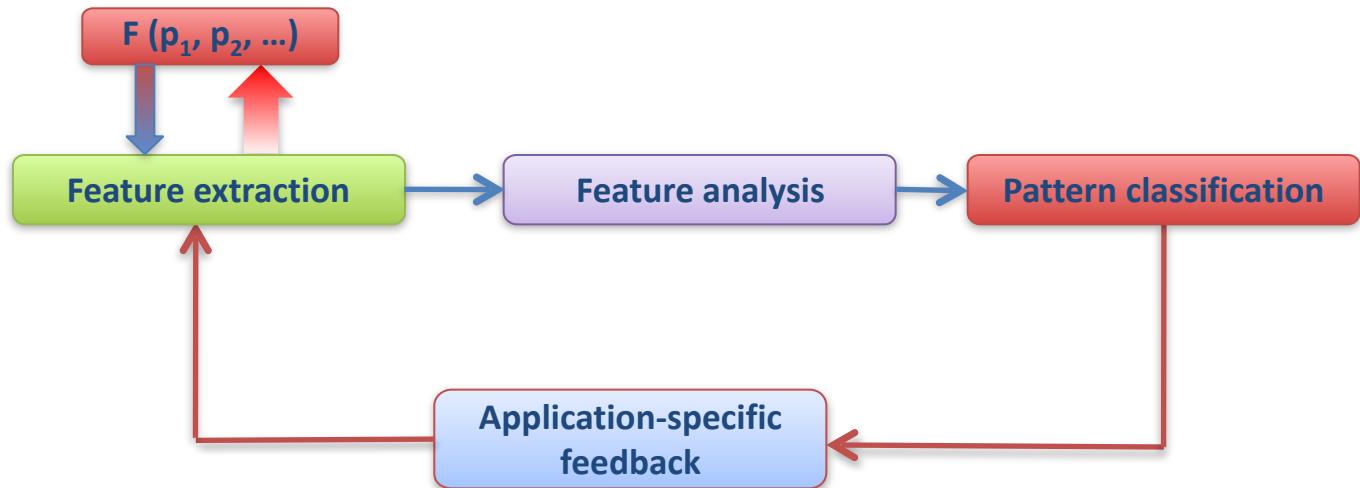
Find if:

- A, B, ...N are statistically **identical**
- A, B, ...N are statistically **different** and **quantify** the difference.

Pattern recognition process



Pattern recognition process

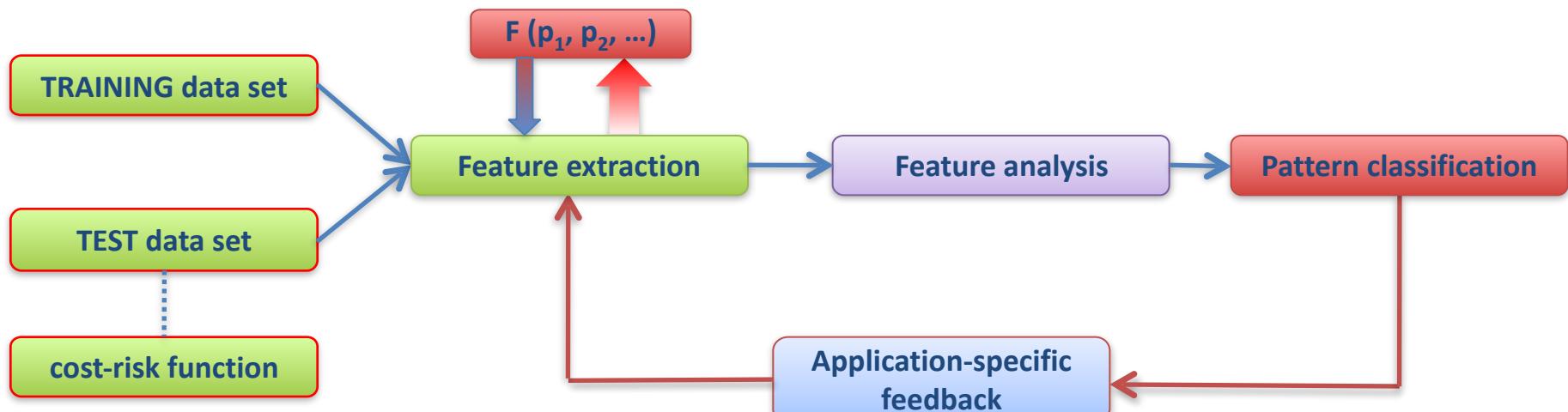


The final **results** from pattern recognition can be used **as input** to automatically **re-define the parameters p_i** of feature extraction operators.

This procedure can be **iteratively repeated** to improve the feature extraction process.

**MACHINE
LEARNING**

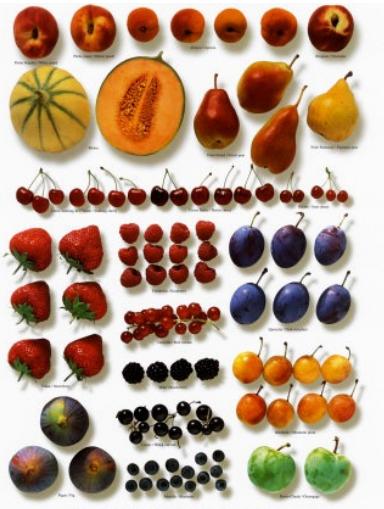
Pattern recognition process



The final **results** from pattern recognition can be used **as input** to automatically **re-define the parameters p_i** of feature extraction operators.

This procedure can be **iteratively repeated** to improve the feature extraction process.

**MACHINE
LEARNING**

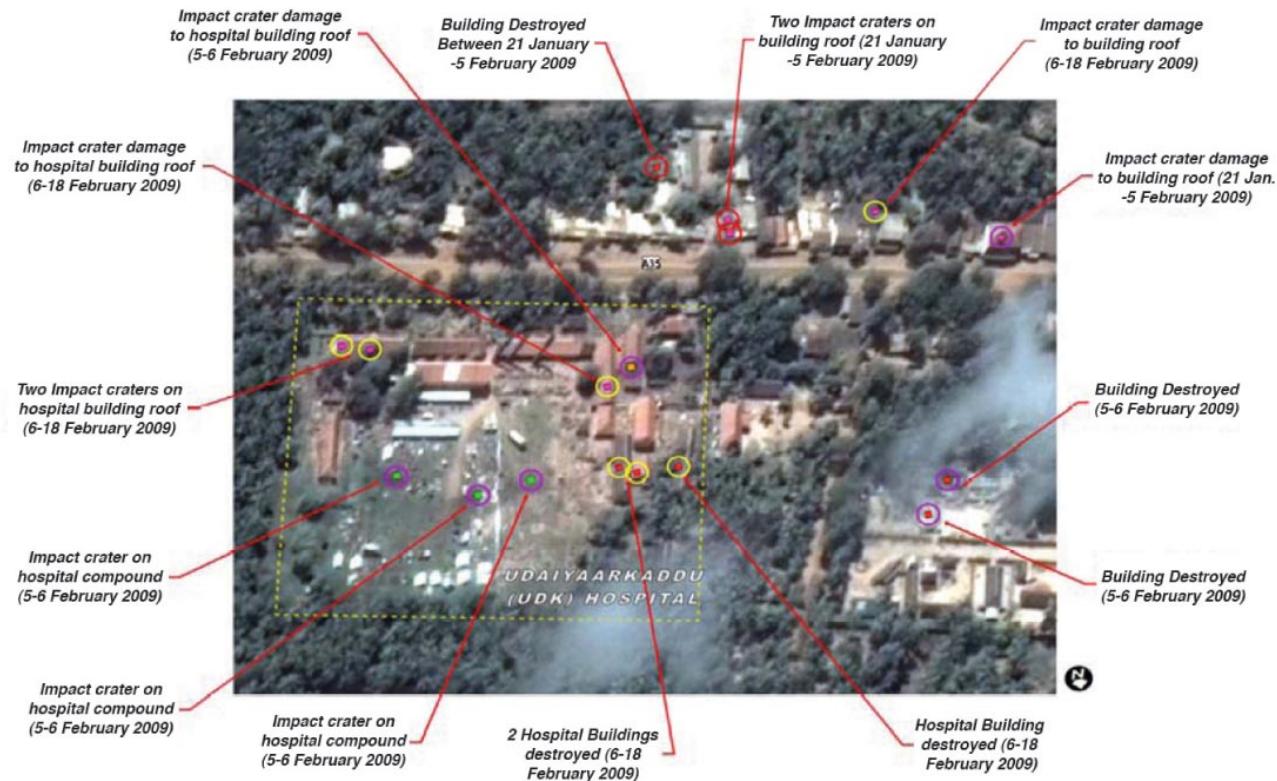


Pattern recognition process

	peach		prune
	melon		apple
	sliced melon		cassis
	pear		strawberry
	fig		raspberry
	apricot		blueberry
	cherries		blackberry
	red currant		

Military applications

Used to discover enemy targets over satellite maps or check the air raids and bombing



Darusman Report commissioned by UN, Sri Lanka

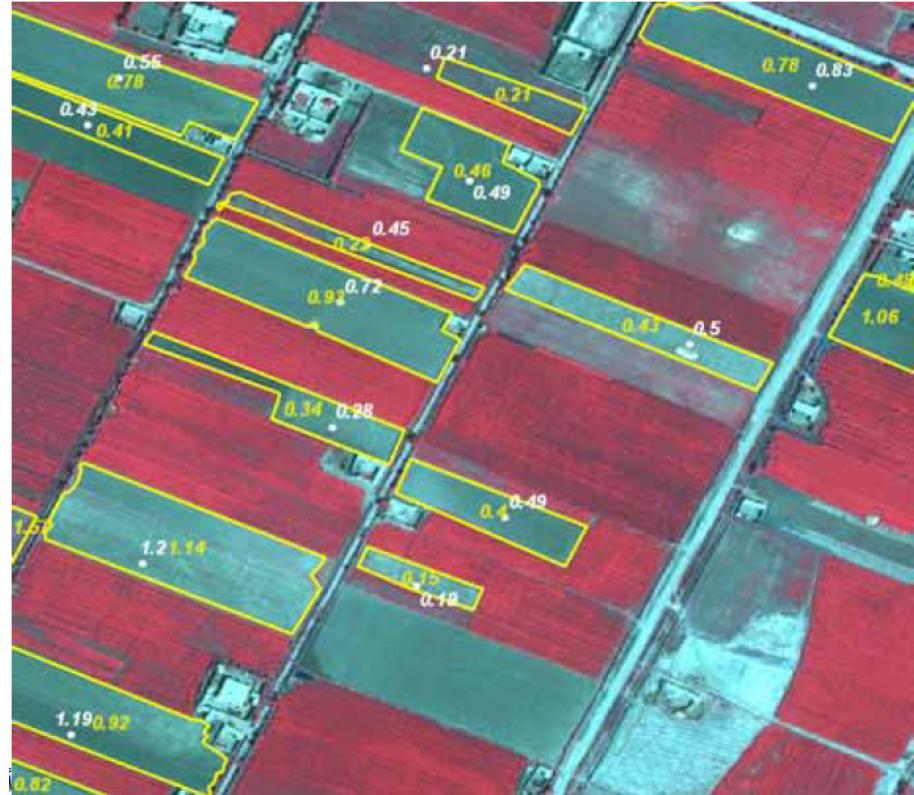
<http://www.thesundayleader.lk/wp-content/uploads/2011/04/map.jpg>

Opium cultivated areas

Nad Ali district, Hilmand province, Afghanistan



Satellite image with pattern recognition of opium cultivated areas



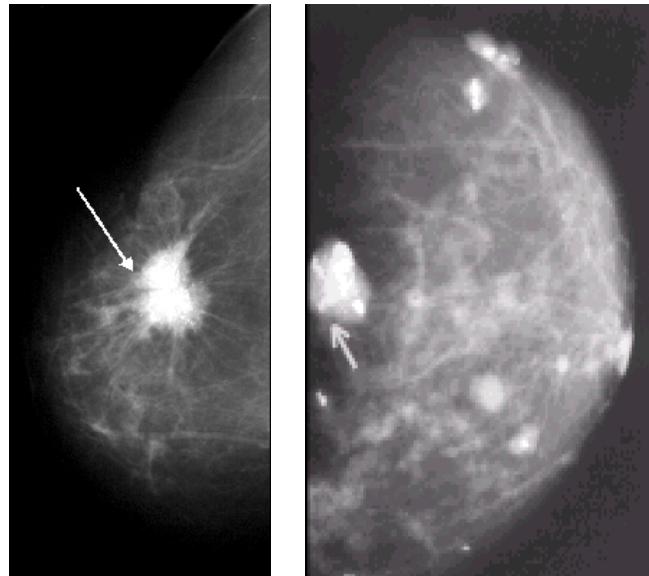
Satellite image with pattern classification (areas in ha) of opium cultivated/eradicated areas

Medical applications

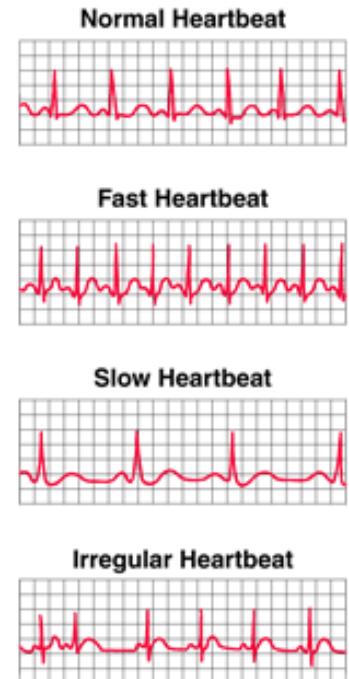
Alzheimer disease



Breast cancer



ECG pattern



Jan Klohs et al.,
J Cereb Blood Flow Metab. 2011
Aug 17;

Stefan Kloßapel, et al.,
Brain (2008), 131, 6810689

<http://www.szote.u-szeged.hu/radio/emlo/aemlo6a.htm>
Gebrim LH, Sao Paulo Med J. 2000 Mar 2;118(2):46-8.

Desok Kim et al.,
2008 International Conference on
BioMedical Engineering and Informatics

Data Integration

complexity

Spatial domain \Re^3

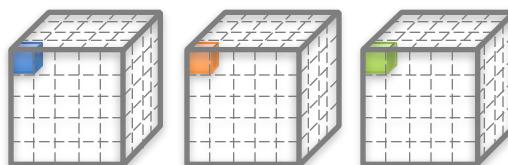
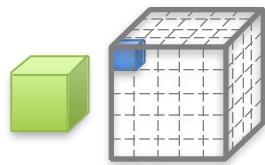
Spatial domain \Re^3

Features domain \Re^N

Spatial domain \Re^3

Features domain \Re^N

Time domain \Re^1



Shape analysis

Texture analysis

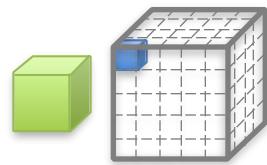
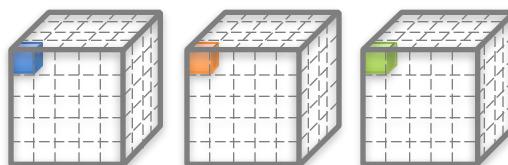
Complex Network

Pattern recognition

Clustering

Data Integration

complexity

Spatial domain \Re^3 Spatial domain \Re^3 Features domain \Re^N Spatial domain \Re^3 Features domain \Re^N Time domain \Re^1 

Shape analysis

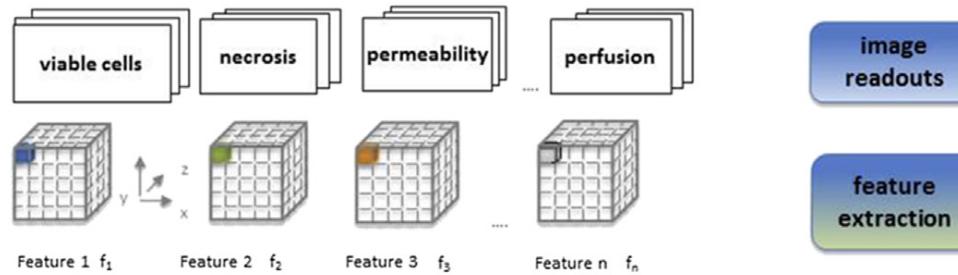
Texture analysis

Complex Network

Pattern recognition

Clustering

Imaging to Network

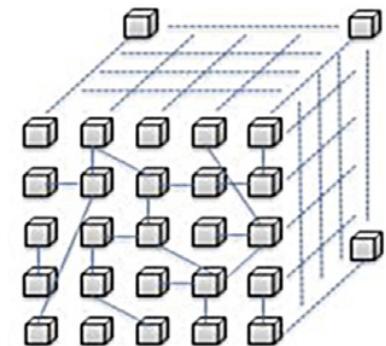


The **nodes** are identified by the voxel and described by the features $F_1 F_2 F_3 \dots F_M$

$$n_{x,y,z} \equiv v(F_1, F_2, F_3, \dots, F_M)_{x,y,z}$$

The **edges** (links) between the nodes are determined on the basis of **similarity** between the nodes

$$E_{n_i, n_k} \equiv \Theta \left[C_{N_T, 2}^{i=1 \rightarrow N_T, k=1 \rightarrow N_T} (n_i, n_k) \right]$$



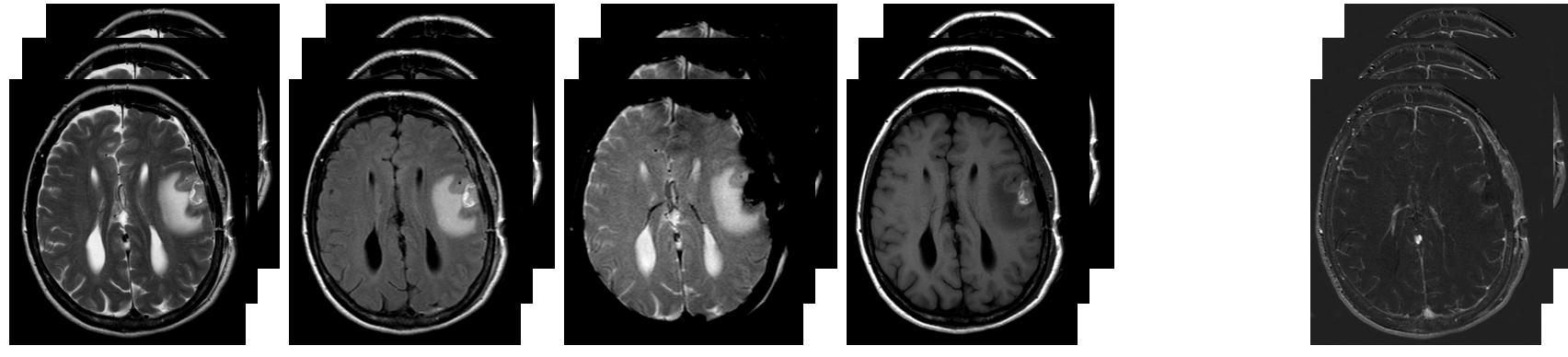
All the edges form the **adjacency matrix**

$$M \equiv E_{n_i, n_k} \Big|_{\substack{i=1 \rightarrow N_T \\ k=1 \rightarrow N_T}}$$

Integrative analysis of cancer imaging readouts by networks

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Molecular Oncology, Volume 9, Issue 1, January 2015, Pages 1–16



sT2-TSET-sense
Feature 1

sT2w-FLAIR
Feature 2

T2w- FE-EPI
Feature 3

T-SE-pre Gadolinium
Feature 4

Sous-angiography
Feature 7

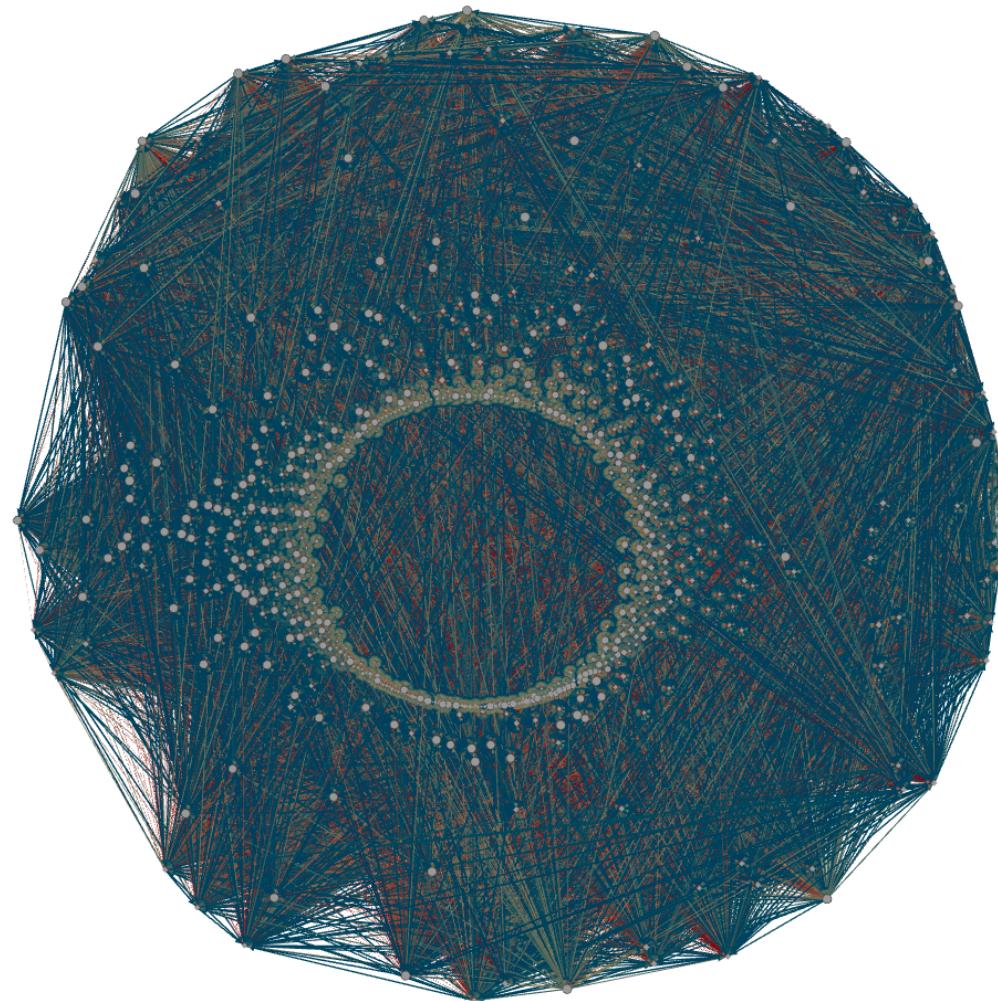
.....

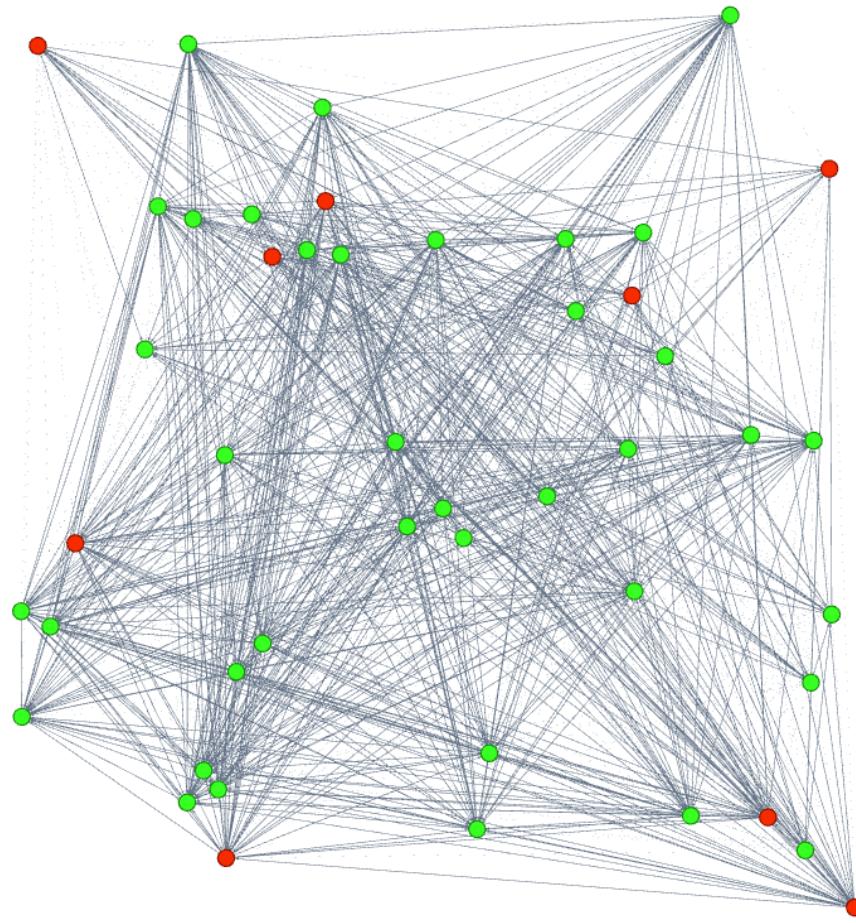
3D Regions of interest including:

- Tumor tissue
- Healthy tissue 1cm

BRAINX dataset from Osirix database



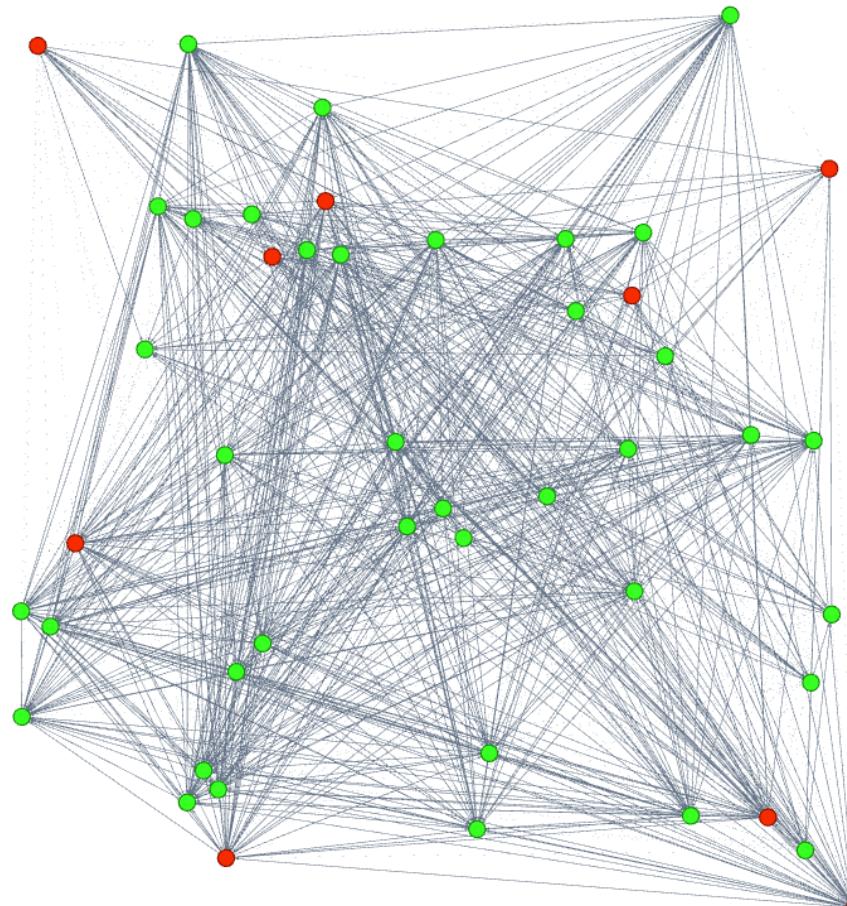




Small 3D ROI subset

Nodes: 47
Edges: 1081
Directed Graph

- Tumor
- Healthy tissue



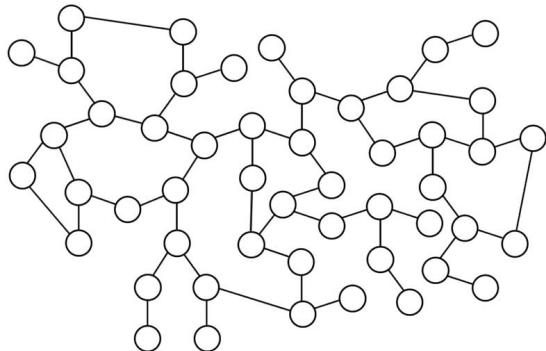
Small 3D ROI subset

Nodes: 47
Edges: 1081
Directed Graph

- Tumor
- Healthy tissue

What is the information behind nodes and edges
in clinical terms?

Random network



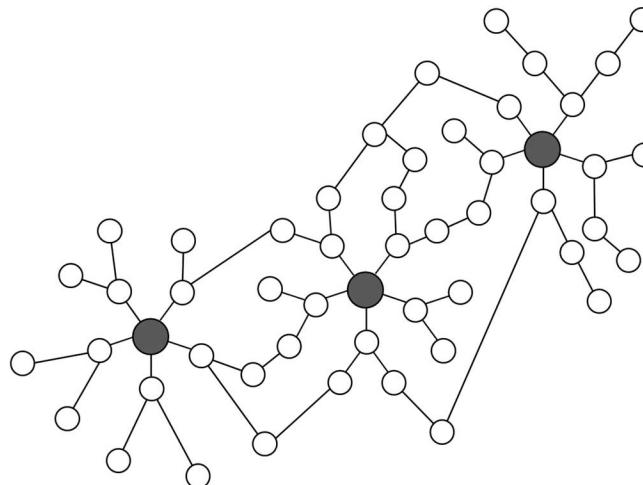
Follow **Poisson** distribution

Homogeneous structure

Nodes have almost the same number of edges

Examples: secondary roads networks

Scale-free network



Follow **Power Law** distribution

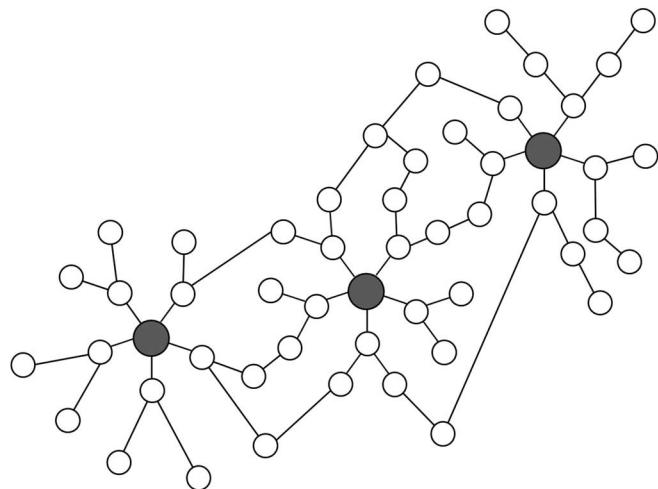
Inhomogeneous structure

Nodes have different number of edges

Example: airlines networks, social networks, biological networks, etc.

Scale-free network

Network dynamic is governed by **physiological rules**.



Authorities

Authorities are nodes that contains useful information on the network behavior

Example: web pages

Hubs

Hubs are nodes that tell us where the best authorities are to be found

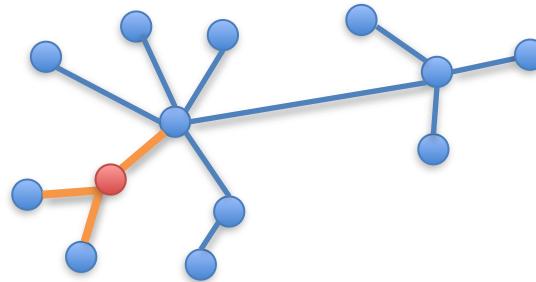
Example: google search results

Metrics/statistics

Centrality

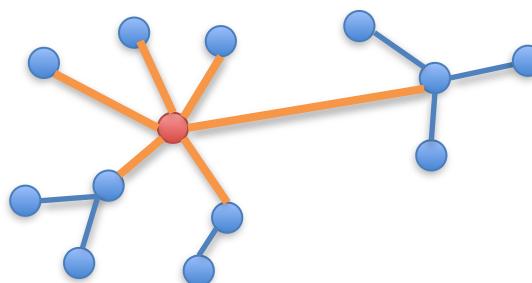
For a given node, centrality measures the number of nodes connected to it

- centrality degree
- eigenvecor centrality
- katz centrality
- Page Rank

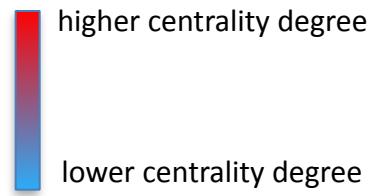
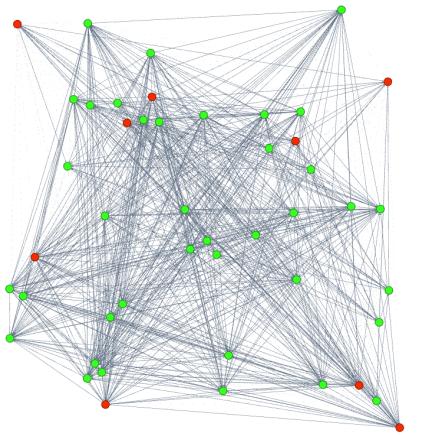


Closeness centrality

For a given node, closeness centrality measures the mean distance with the other nodes (based on feature similarity).



Goal: evaluate **nodes hierarchy**

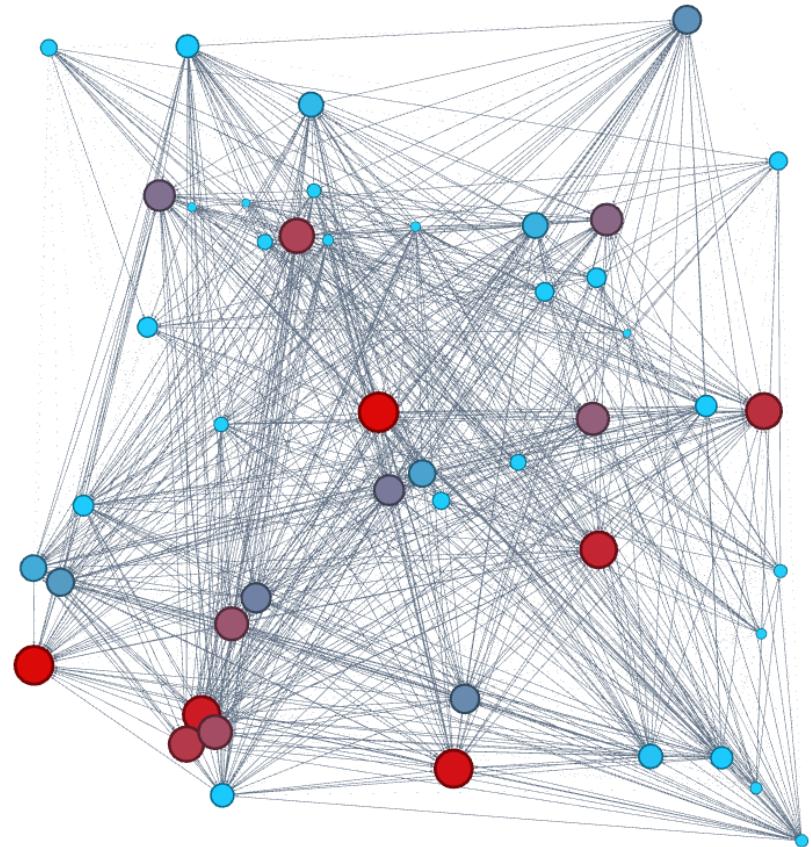


Nodes higher number of edges/connections have higher importance

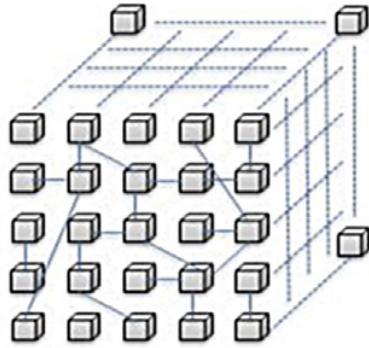
They control the majority of the other nodes

target for therapy

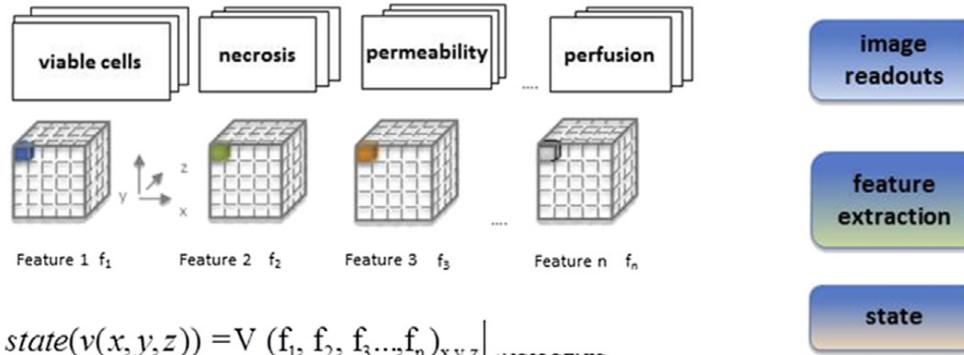
Nodes hierarchy



State



Based on features value, for each nodes is possible to define a **state**



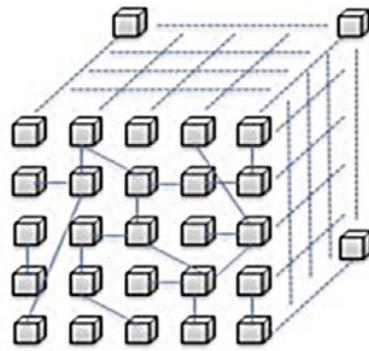
$$state(v(x,y,z)) = V(f_1, f_2, f_3, \dots, f_n)_{x,y,z} \Big|_{ANGIOGENIC}$$

$$state(v(x,y,z)) = V(f_1, f_2, f_3, \dots, f_n)_{x,y,z} \Big|_{NON-ANGIOGENIC}$$

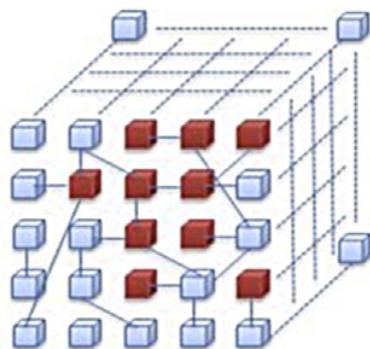
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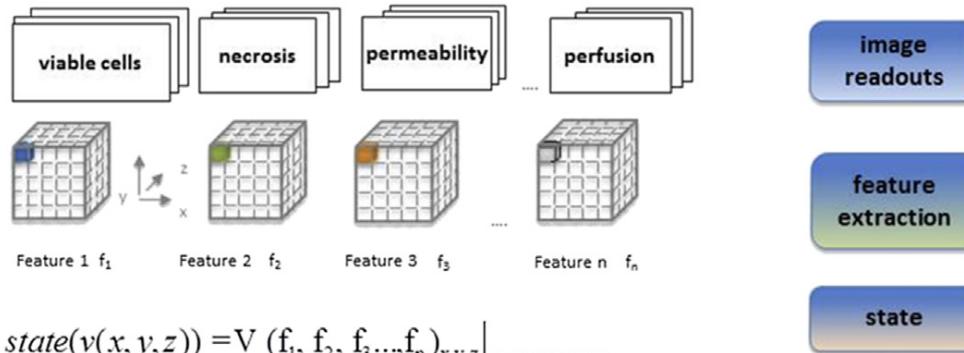


Voxel Clustering



State

Based on features value, for each nodes is possible to define a **state**



Nodes in the same state can be grouped in **clusters**

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Results: macroscopic level

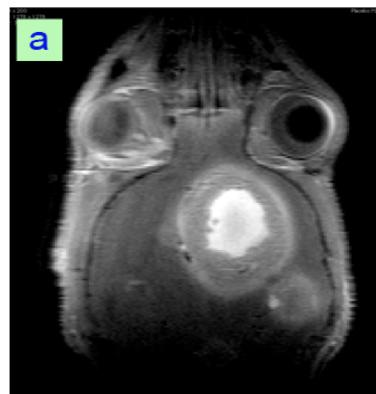
Table 1 – List of features characterizing tumor tissues (left), and corresponding MI modality through which feature measurements are obtained (middle). References are reported for each example.

Features	MI modality	Reference
Morphology:		
shape	MRI (T_1 , T_2 , ρ), CT	(Young, 2007)
solid vs liquid regions	MRI (T_1 , T_2 , ρ), CT	(Young, 2007)
necrotic regions	MRI (T_1 , T_2 , ρ), CT	(Berry et al., 2008)
viable regions	MRI (T_1 , T_2 , ρ)	(Berry et al., 2008)
alteration in cellularity	MRI – ADC	(Drevelegas, 2011; Haacke, 1999)
apoptosis	PET (^{124}I -annexin V)	(Blankenberg, 2008)
Inflammatory status		
edema formation	MRI (T_1 , T_2 , FLAIR), CT	(Young, 2007)
infiltration of immune cells	MRI (cell tracking SPIO)	(Bulte, 2009; Ahrens and Bulte, 2013)
Physiology		
angiogenesis	MRI (DCE)	(Barrett et al., 2007)
vascular architecture	CT (angiography), MRI (angiography)	(Matsumotoa et al., 2007; Hartung et al., 2011)
vessel density	MRI (VSI)	(Barrett et al., 2011)
hemodynamic response	MRI (DSC)	
vascular permeability	MRI (DCE)	
tumor oxygenation	PET (^{18}F -MISO), MRI (BOLD, ^{17}O)	
acidosis	MRI, MRS	
Tumor metabolism		
glucose consumption	^{18}FDG PET	
metabolites concentration	MRS	

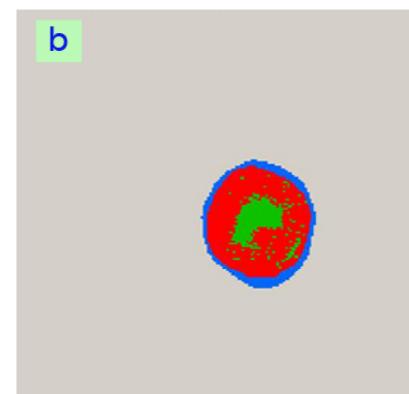
Three types of tissue in a different state

- S1 --> highly angiogenic
- S2 --> proliferating tissue
- S3 --> necrotic tissue

placebo



MRI



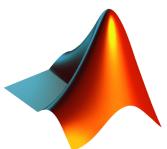
Clustering

Quantification of antiangiogenic treatment effects on tissue heterogeneity in glioma tumor model
 Marco Dominietto, Sandra Bürgi, Michael Dobosz, Anja Renner, Gudrun Zahlmann, Werner Scheuer and Markus Rudin
Submitted manuscript

Pattern Recognition



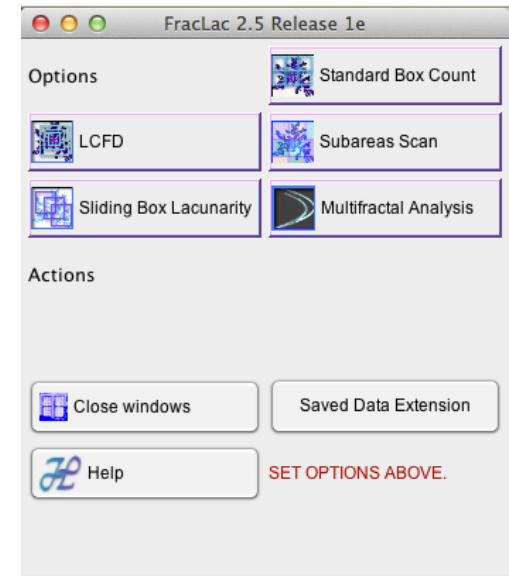
ImageJ
Image Processing and Analysis in Java



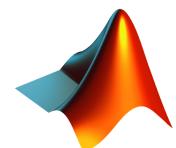
MATLAB®
The Language of Technical Computing



Boxcount toolbox



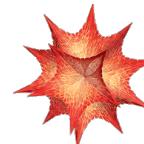
Complex Network



MATLAB®
The Language of Technical Computing



C++ Java



MATHEMATICA®5



Data Integration

complexity

Spatial domain \Re^3

Spatial domain \Re^3

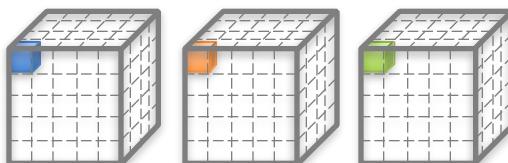
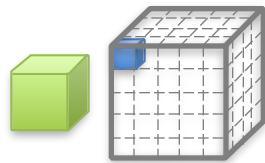
Features domain \Re^N

Spatial domain \Re^3

\Re^3

Features domain \Re^N

\Re^1



Shape analysis

Texture analysis

Complex Network

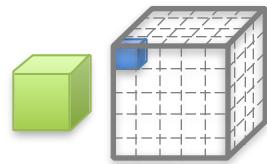
Pattern recognition

Clustering

Data Integration

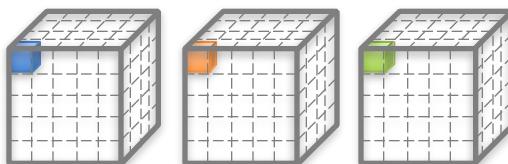
complexity

Spatial domain \mathbb{R}^3



Spatial domain \mathbb{R}^3

Features domain \mathbb{R}^N



Spatial domain \mathbb{R}^3

Features domain \mathbb{R}^N

Time domain \mathbb{R}^1



Shape analysis

Texture analysis

Complex Network

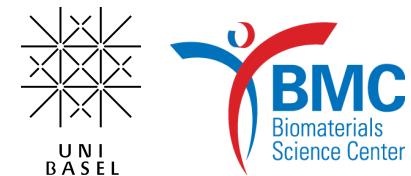
Pattern recognition

Clustering

“...In the era of internet, the real knowledge does not come from the amount of information we are able to process, but from the number of connections we are able to establish among them”.

Somewhere in the web

Acknowledgments



People from:

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Enrico Capobianco

Center for Computational Science, University of Miami,
Miami, FL, (USA)



Giulio Magrin

MedAustron, Wiener Neustadt (Austria)



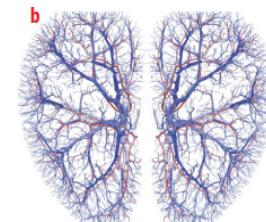
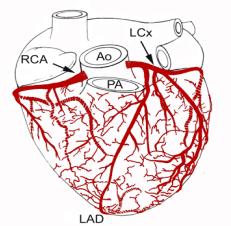
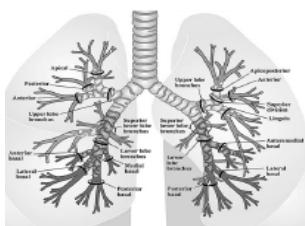
Several example in nature:



Several example in living organism:



Several example in human body:



Several example in human
“constructions”:

