

Inverse Problems for Biomedical Systems

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Model : RTE

Evaluation of the integral

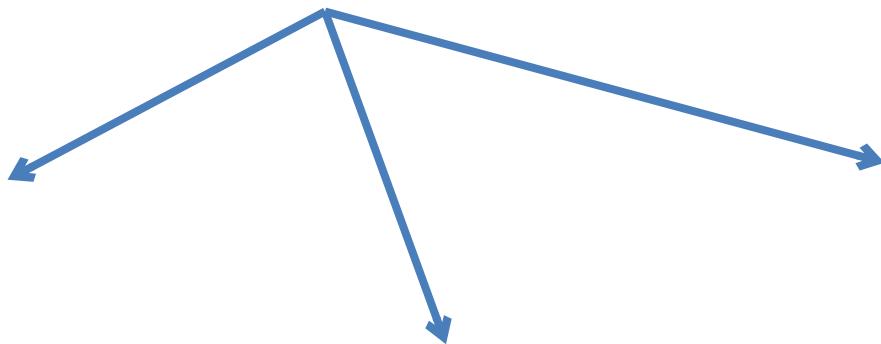
$$\frac{1}{c} \frac{\partial L_\nu(s, \mathbf{u}, t)}{\partial t} + \mathbf{u} \cdot \nabla L_\nu(s, \mathbf{u}, t) = -(\mu_a + \mu_s)L_\nu(s, \mathbf{u}, t) + \frac{\mu_s}{4\pi} \int_{4\pi} p h_\nu(s, \mathbf{u}', \mathbf{u}) L_\nu(s, \mathbf{u}', t) d\Omega' ds + Q(\mathbf{r}, \mathbf{u}, t)$$

Developments:

PN Approximations
P1: Diffusing wave theory
P3:
Diffusion Approximation

Stochastics

Monte Carlo simulations
Random walk



Discretizations (space, angular)
Discrete Ordinates Method(DOM=SN)
Kubelka-Munk (2Flux)
Adding-doubling
FDM,FEM

+ Hybrid Methods

Case 1: Non-scattering media

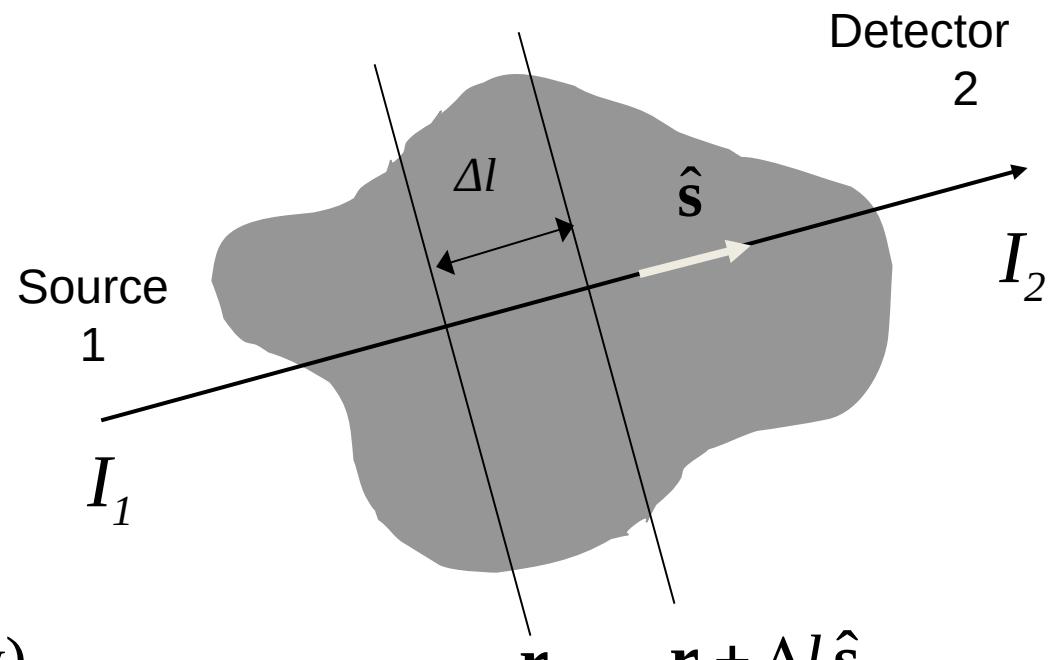
X-ray propagation

- X-rays propagate along straight lines
- Suffer absorption along their paths

$$I(\mathbf{r} + \Delta l \hat{\mathbf{s}}) = I(\mathbf{r}) e^{-\alpha(\mathbf{r}) \Delta l} \quad (\text{Beer's law})$$

$$\frac{dI(\mathbf{r})}{ds} = -\alpha(\mathbf{r}) I(\mathbf{r}) \Leftrightarrow \hat{\mathbf{s}} \cdot \nabla I + \alpha(\mathbf{r}) I(\mathbf{r}) = 0$$

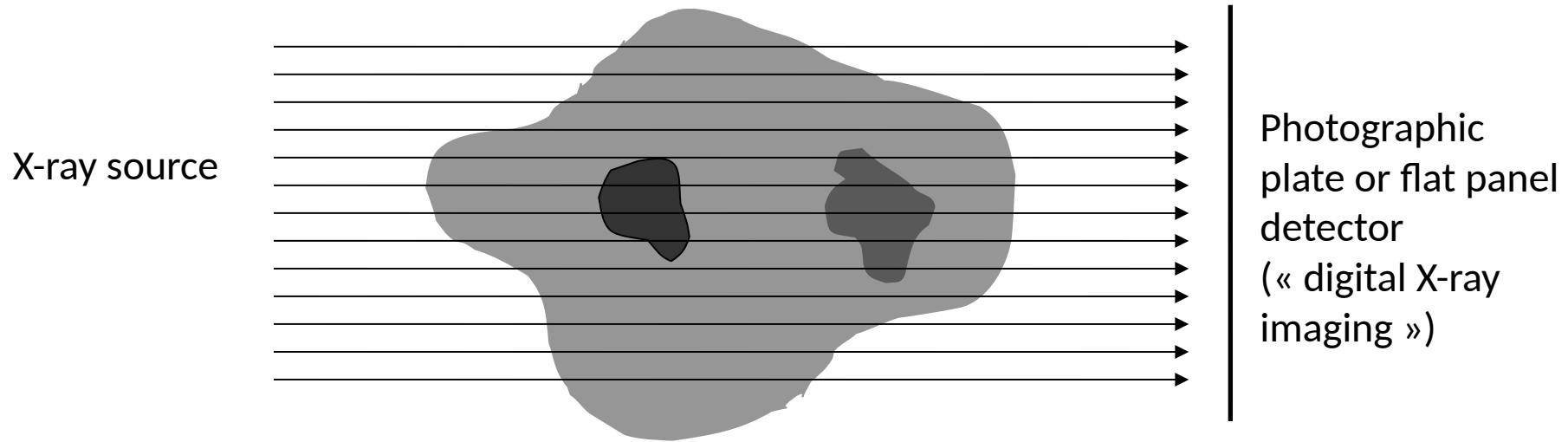
$$\Rightarrow -\ln\left(\frac{I_2}{I_1}\right) = \int_1^2 \alpha(\mathbf{r}) dl \quad (\text{line integral})$$



$$I(\mathbf{r}) \quad I(\mathbf{r} + \Delta l \hat{\mathbf{s}})$$

$\hat{\mathbf{s}}$ = unit vector
along the straight line

Traditional X-ray imaging



- Problem: All the information acquired along a ray is projected on a single point on the photographic plate (or flat panel electronic detector nowadays)

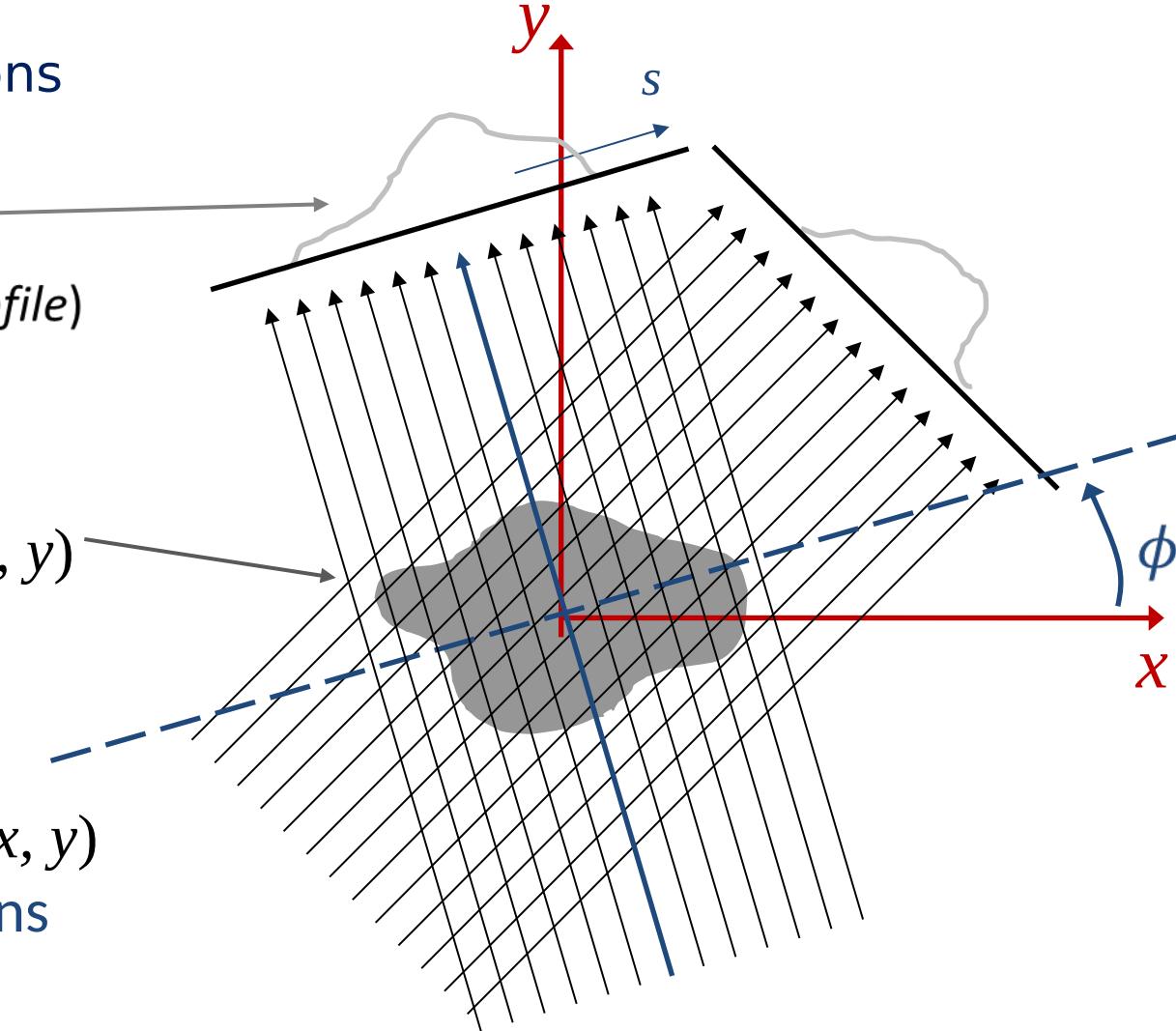
X-ray computed tomography (CT)

- Parallel projections

Projection $p(s, \phi)$

(*~transmitted intensity profile*)

Object $\alpha(x, y)$

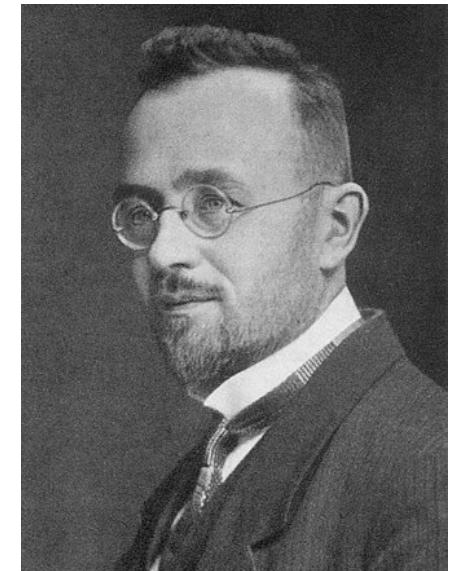
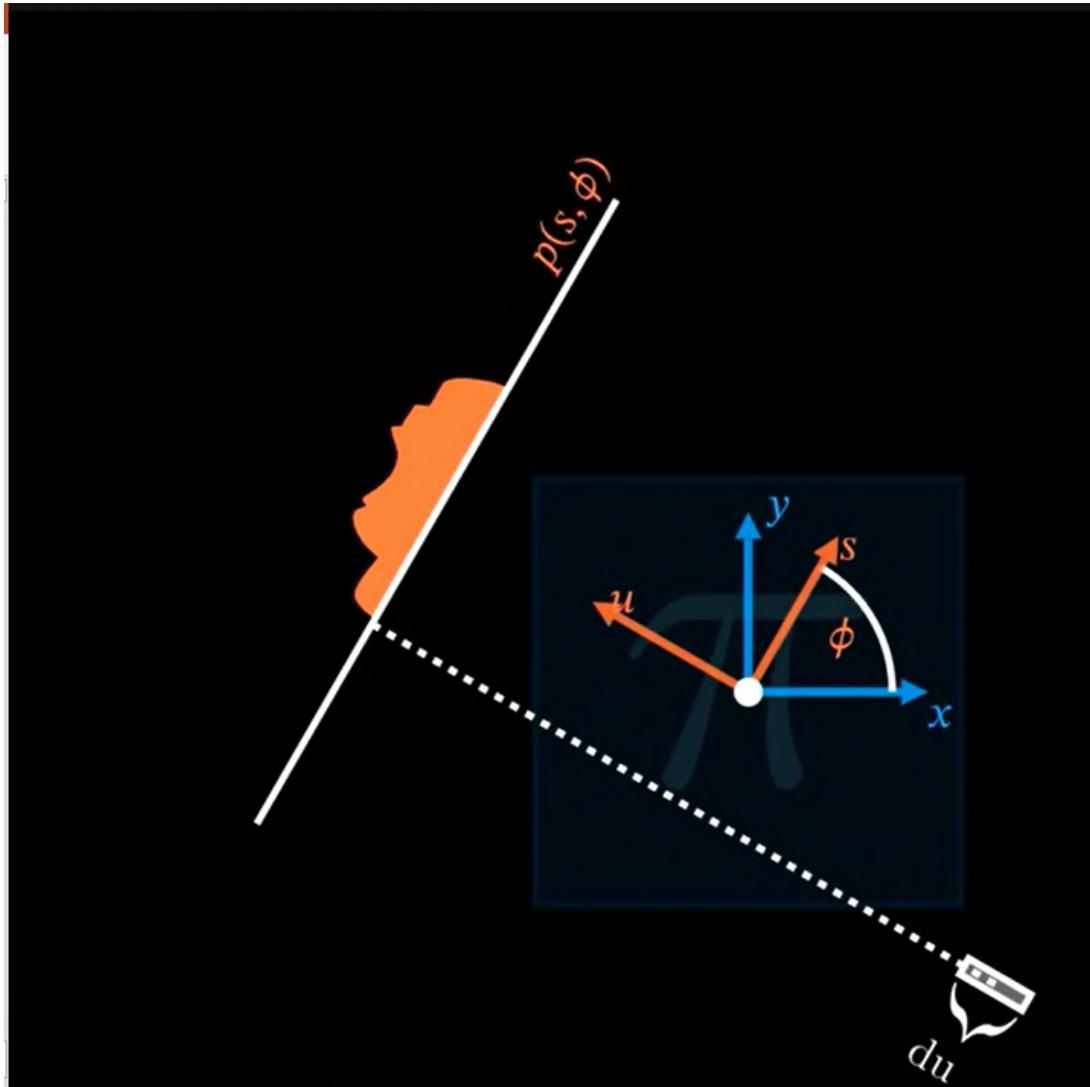


Goal of CT: recover $\alpha(x, y)$
from several projections

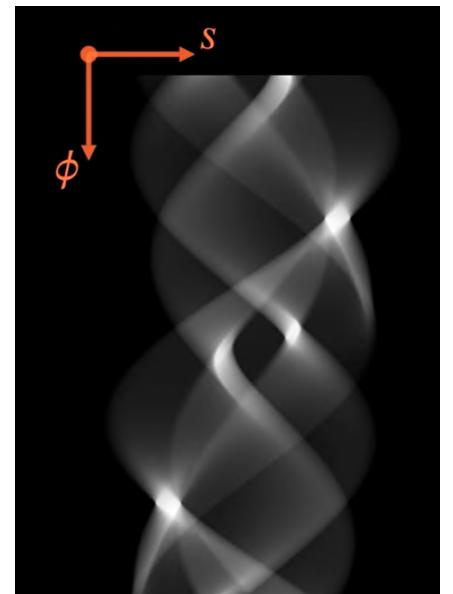
Radon Transform : $F = \mathcal{R}$

Johann Radon (1887-1956)

1917



Sinogram

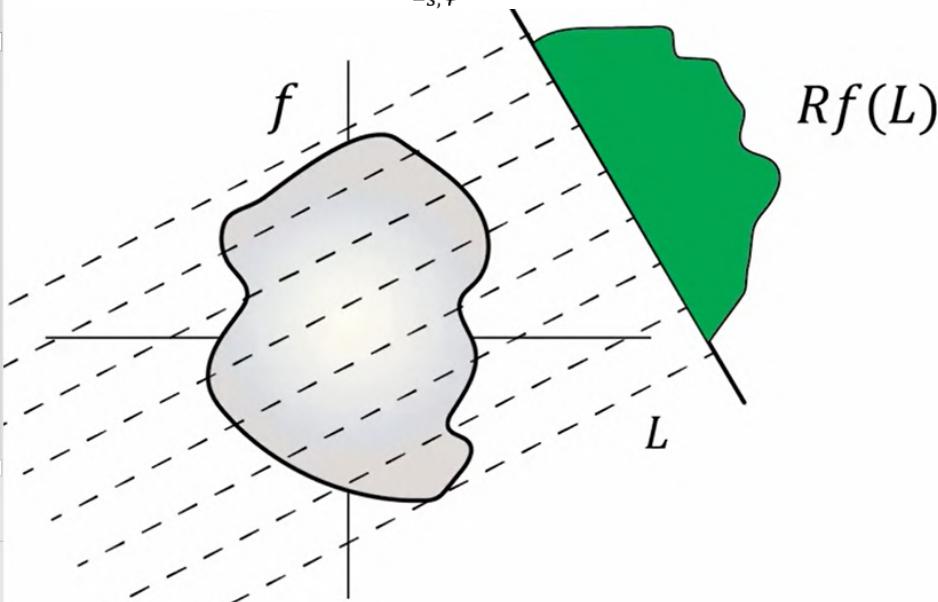
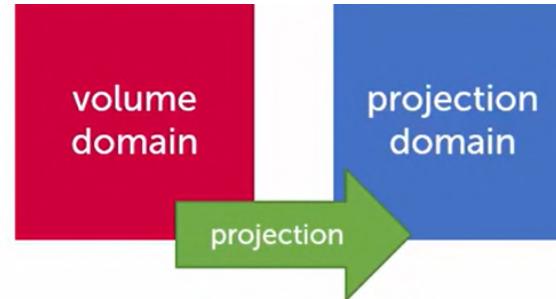


Solving an inverse problem

Analytical vs Algebraic

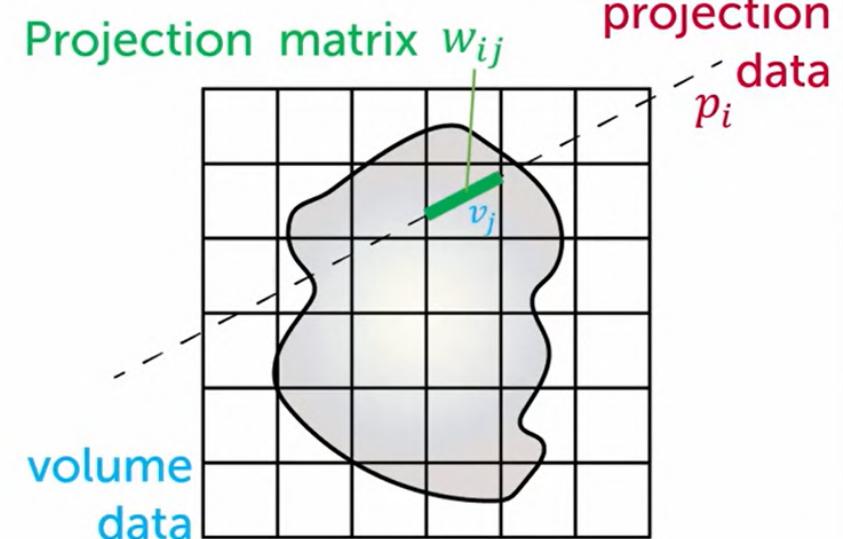
analytically

$$p(s, \phi) = \mathcal{R}\{f(x, y)\} = \int_{L_s, \phi} f(x, y) du$$



algebraically

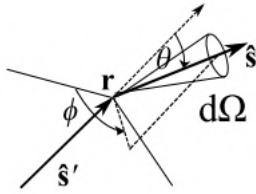
$$p = Wv$$



Case 2: Highly-scattering media

Diffusion Approximation

1-Model: From RTE to DE



Expansion of the Radiance in Spherical Harmonics $Y_{n,m}(\theta, \phi)$

$$L(\mathbf{r}, \hat{\mathbf{s}}, t) = \sum_{n=0}^{\infty} \sum_{m=-n}^n L_{n,m}(\mathbf{r}, t) Y_{n,m}(\hat{\mathbf{s}})$$

Ex.

$$Y_{0,0}(\theta, \phi) = \frac{1}{\sqrt{4\pi}},$$

$$Y_{1,-1}(\theta, \phi) = \sqrt{\frac{3}{8\pi}} \sin \theta e^{-i\phi},$$

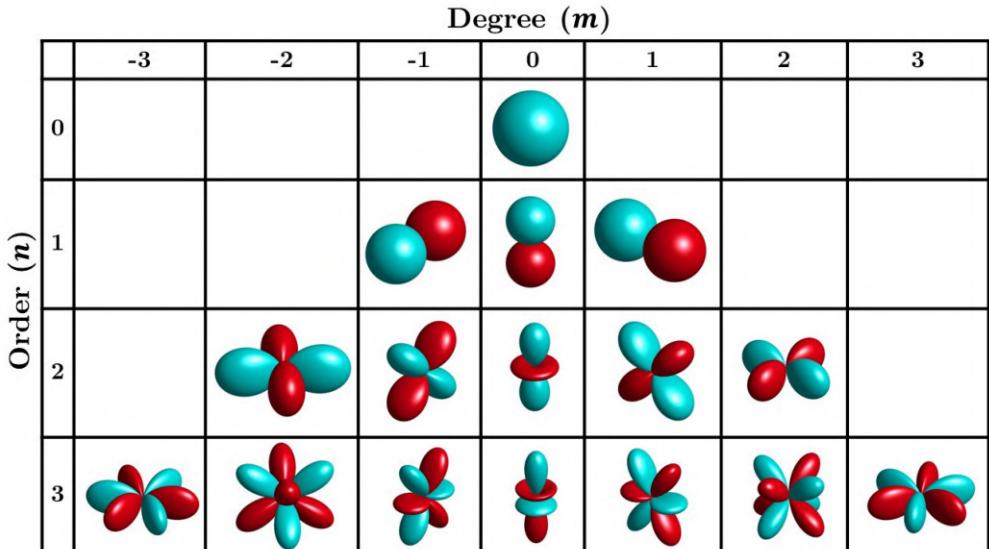
$$Y_{1,0}(\theta, \phi) = \sqrt{\frac{3}{4\pi}} \cos \theta,$$

$$Y_{1,1}(\theta, \phi) = -\sqrt{\frac{3}{8\pi}} \sin \theta e^{i\phi}.$$

Truncation at order N: « PN approximation »

SH orthogonality property:

$$\int_{4\pi} Y_{n,m}(\hat{\mathbf{s}}) Y_{n',m'}^*(\hat{\mathbf{s}}) d\Omega = \int_0^{2\pi} \int_0^\pi Y_{n,m}(\theta, \phi) Y_{n',m'}^*(\theta, \phi) \sin \theta d\theta d\phi = \delta_{n,n'} \delta_{m,m'}$$



Diffusion Approximation

$$L_{n,m}(\mathbf{r}, t) = \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) Y_{n,m}^*(\hat{\mathbf{s}}) d\Omega$$

P1 approximation

$$L(\mathbf{r}, \hat{\mathbf{s}}, t) = L_{0,0}(\mathbf{r}, t) Y_{0,0}(\hat{\mathbf{s}}) + L_{1,1}(\mathbf{r}, t) Y_{1,1}(\hat{\mathbf{s}}) + L_{1,-1}(\mathbf{r}, t) Y_{1,-1}(\hat{\mathbf{s}})$$

(1) \rightarrow

$$\begin{aligned} L_{0,0}(\mathbf{r}, t) &= \int_{4\pi}^{(1)} L(\mathbf{r}, \hat{\mathbf{s}}, t) Y_{0,0}^*(\hat{\mathbf{s}}) d\Omega \\ &= \int_{4\pi}^{(2)} L(\mathbf{r}, \hat{\mathbf{s}}, t) \frac{1}{\sqrt{4\pi}} d\Omega \\ &= \frac{1}{\sqrt{4\pi}} \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) d\Omega = \frac{\phi(\mathbf{r}, t)}{\sqrt{4\pi}} \quad \text{Fluence Rate [W.m}^{-2}\text{]} \end{aligned}$$

(2) $\hat{\mathbf{s}} = (s_x, s_y, s_z) = (\sin \theta \cos \phi, \sin \theta \sin \phi, \cos \theta)$ **Current Density Vector [W.m⁻²]:** $\mathbf{J}(\mathbf{r}, t) = \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) \hat{\mathbf{s}} d\Omega$

$$Y_{1,-1}(\theta, \phi) = \sqrt{\frac{3}{8\pi}} (s_x - i s_y), \quad L_{1,-1} = \sqrt{\frac{3}{8\pi}} \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) (s_x + i s_y) d\Omega$$

$$Y_{1,0}(\theta, \phi) = \sqrt{\frac{3}{4\pi}} s_z, \quad L_{1,0} = \sqrt{\frac{3}{4\pi}} \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) s_z d\Omega$$

$$Y_{1,1}(\theta, \phi) = -\sqrt{\frac{3}{8\pi}} (s_x + i s_y) \quad L_{1,1} = -\sqrt{\frac{3}{8\pi}} \int_{4\pi} L(\mathbf{r}, \hat{\mathbf{s}}, t) (s_x - i s_y) d\Omega$$

$$\mathbf{J} = \sqrt{\frac{2\pi}{3}} (L_{1,-1} - L_{1,1}, -i(L_{1,-1} + L_{1,1}), \sqrt{2}L_{1,0})$$

$$J_x = \sqrt{\frac{2\pi}{3}} (L_{1,-1} - L_{1,1}),$$

$$J_y = -i \sqrt{\frac{2\pi}{3}} (L_{1,-1} + L_{1,1}),$$

$$J_z = \sqrt{\frac{4\pi}{3}} L_{1,0},$$

$$\mathbf{J} \cdot \hat{\mathbf{s}} = \sqrt{\frac{2\pi}{3}} \sum_{m=-1}^1 L_{1,m}(\mathbf{r}, t) Y_{1,m}(\hat{\mathbf{s}})$$



$$\text{P1 approximation: } L(\mathbf{r}, \hat{\mathbf{s}}, t) = \frac{\phi(\mathbf{r}, t)}{\sqrt{4\pi}} + \frac{3}{4\pi} \mathbf{J} \cdot \hat{\mathbf{s}}$$

Diffusion Equation

Combination of

$$\left\{ \begin{array}{l} \int_{4\pi} (RTE) ds \\ \int_{4\pi} (RTE).sds \end{array} \right. \quad \begin{array}{l} \frac{1}{c} \frac{\partial}{\partial t} \phi(\mathbf{r}, t) + \nabla \cdot \mathbf{J} + \mu_a(\mathbf{r}) \phi(\mathbf{r}, t) = Q(\mathbf{r}, t) \\ + \text{additional assumptions} \\ \frac{1}{c} \frac{\partial}{\partial t} \mathbf{J}(\mathbf{r}, t) + \frac{1}{3} \nabla \phi(\mathbf{r}, t) + [\mu_a(\mathbf{r}) + \mu'_s(\mathbf{r})] \mathbf{J}(\mathbf{r}, t) = 0 \\ \mathbf{J}(\mathbf{r}, t) = -D \nabla \phi(\mathbf{r}, t) \text{ Fick's law} \end{array}$$

+ additional assumptions =

Diffusion Approximation (DA) $\left| \frac{1}{c} \frac{\partial}{\partial t} \mathbf{J}(\mathbf{r}, t) \right| \ll (\mu_a + \mu'_s) |\mathbf{J}(\mathbf{r}, t)|$ ↪ Slowly varying phenomena

$$\mu' \equiv \mu_s(1-g) \quad \text{Reduced scattering coefficient}$$

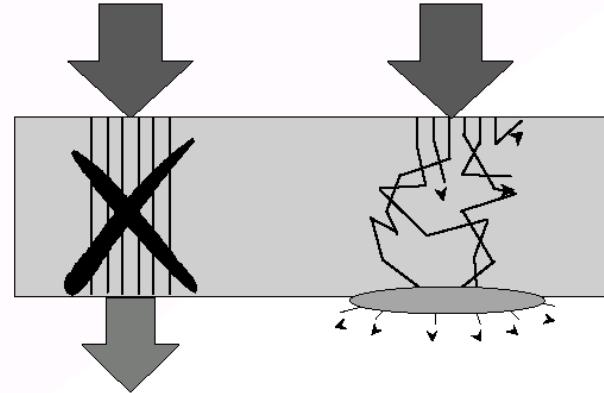
$$D = \frac{1}{3(\mu'_s + \mu_a)} \quad \text{Diffusion coefficient}$$



$$\frac{1}{c} \frac{\partial}{\partial t} \phi(\mathbf{r}, t) - \nabla \cdot (D(\mathbf{r}) \nabla \phi(\mathbf{r}, t)) + \mu_a(\mathbf{r}) \phi(\mathbf{r}, t) = Q(\mathbf{r}, t)$$



Absorption (μ_a)



Diffusion (μ_s')

$$-\nabla \cdot \left(\frac{1}{3\mu_s(r)} \nabla \phi(r, t) \right) + \frac{1}{v} \frac{\partial}{\partial t} \phi(r, t) + \mu_a(r) \phi(r, t) = S(r, r_0, t)$$

Diffusion

Propagation

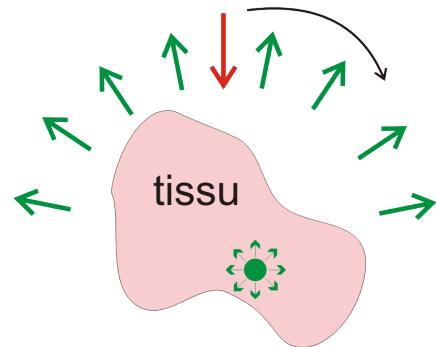
Absorption

Source

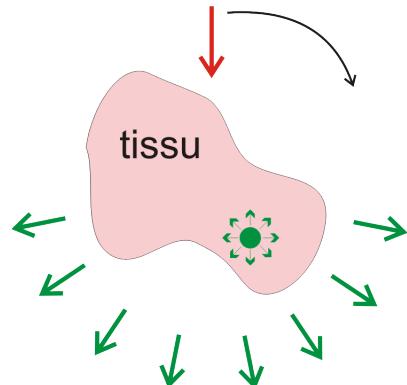
Several configurations are possible

Pogue, et al, Comparison of imaging geometries for DOT of tissue Opt. Expr., 1999, 4, 270-86

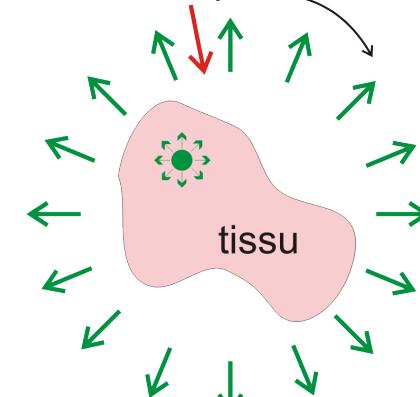
Epi-illumination



Trans-illumination

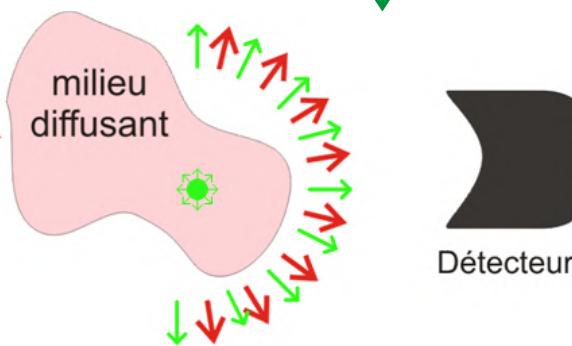


Epi-/Trans-illumination



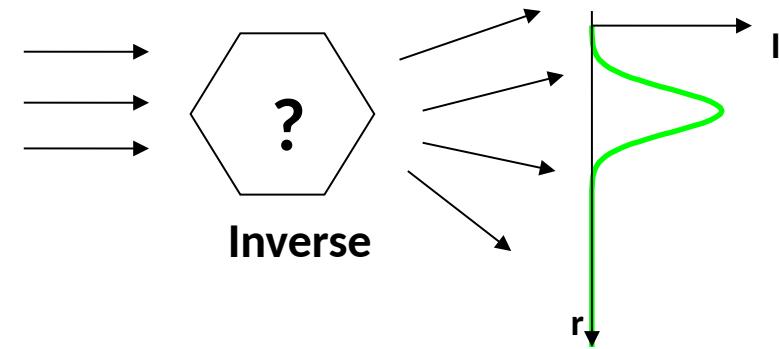
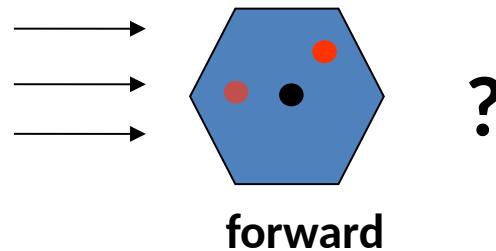
Fluorescence

Source d'excitation
- laser, diode laser
- peut être pulsé ou non



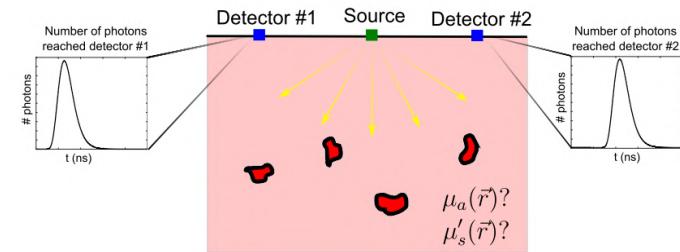
The inverse problem:

Forward problem → Inverse problem



Forward problem:

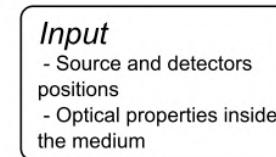
Knowing the **volume** distribution of the unknowns (absorption coefficient, diffusion coefficient, distribution of the markers) → determine profil of **surface** measurements



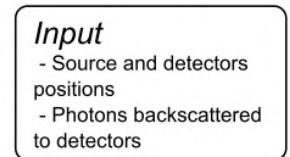
Inverse problem:

Knowing the profil of **surface** measurements → determine **volume** distribution of the unknowns (absorption coefficient, diffusion coefficient, distribution of the markers)

Forward problem



Inverse problem



Principal problem: # of unknowns > # of measurements

→ Ill-posed problem

→ Difficulties in determining a unique solution