### **Control and Learning in Biological Systems**

A Dissertation Presented by

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to

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To my father, Dr. Mohammad Sadeghi, who taught me love, trust, and commitment.

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## **List of Acronyms**

- **AUC** Area Under the Curve. The definite integral of a curve that describes the variation of a drug concentration in blood plasma as a function of time.
- **BiTE** Bispecific T Cell Engagers. A type of fusion protein that is designed to harness the power of the immune system to treat cancer. These bispecific molecules are created by linking the targeting regions of two antibodies.
- **IV** Intravenous Existing or taking place within, or administered into, a vein or veins
- **KIH** Knob Into HolesA well-validated heterodimerization technology for the third constant domain of an antibody.
- **LIGO** Laser Interferometer Gravitational-Wave Observatory. The definite integral of a curve that describes the variation of a drug concentration in blood plasma as a function of time.
- **LTI** Linear Time-InveriantIs a system property that produces an output signal from any input signal subject to the constraints of linearity and time-invariance.
- **FDA** Food and Drug Administration. The United States Food and Drug Administration is a federal agency of the Department of Health and Human Services.
- **MDOR** Mathematically Derived Optimal Regimen.
- **MFI** Maximum Fluorescence Intensity. Indicates the maximum light (photons) emitted. Fluorescence is created by the absorption of energy (light) by fluorescent molecules, called fluorophores.
- **MTD** Maximum Tolerated Dose. The maximum tolerated dose is commonly estimated to be the maximum dose that can be administered for the duration of a specific study that will not compromise the survival of the animals by causes other than carcinogenicity.
- **NPI** Nonpharmaceutical Intervention. Actions, apart from getting vaccinated and taking medicine, that people and communities can take to help slow the spread of illnesses like pandemic influenza (flu).
- **ODE** Ordinary Differential Equation. In mathematics, an ordinary differential equation is a differential equation containing one or more functions of one independent variable and the derivatives of those functions.

- **PMP** Pontryagin Maximum Principle. Is used in optimal control theory to find the best possible control for taking a dynamical system from one state to another, especially in the presence of constraints for the state or input controls.
- **QSS** Quasi Steady State. A situation that is changing slowly enough that it can be considered to be constant.
- **RFM** Ribosome Flow Model. A predictive model for the fundamental features of the translation process, including translation rates, protein abundance levels, ribosomal densities and the relation between all these variables.
- **SCID** Severe combined immunodeficiencySCID mice have a genetic immune deficiency that affects their B and T cells. Due to the lack of mature B and T lymphocytes, these mouse models are ideal for xenoengraftment of human cells and tissue.
- **SISO** Single-Input Single-Output. In control theory, a single-input and single-output system is a simple single variable control system with one input and one output.
- **SD** Social Distancing. In public health, social distancing, also called physical distancing, is a set of non-pharmaceutical interventions or measures intended to prevent the spread of a contagious disease by maintaining a physical distance between people and reducing the number of times people come into close contact with each other.
- **TASEP** Totally asymmetric Simple Exclusion ProcessIs a paradigm model in nonequilibrium statistical mechanics. It is a lattice model in which particles hop into a one-dimensional lattice from the left with rate  $\alpha$ , jump along the lattice to the right with rate  $\beta$  and exit from the right with rate
- **TDB** T-cell-Dependent BispecificSimilar to BiTE. A promising cancer immunotherapy that recruit a patient's T cells to kill cancer cells.
- **TME** Tumor Micro-EnvironmentThe ecosystem that surrounds a tumor inside the body.

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### **Abstract of the Dissertation**

### Control and Learning in Biological Systems

by

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Theory and practice are the two fundamental tools in engineering and scientific research. With a great increase of quantitative experiments in biological systems over the past decades, mathematical modeling is able to enhance predictions and generate new hypotheses. A "good" model of a system, that is expected to reproduce the experimental observations, is capable of making predictions outside the previous experimental settings. However, the accuracy of predictions based on mathematical models highly depends on the assumptions used to model the system. The objective of this study is to explore possible approaches to deploy such models in order to find new hypotheses to be tested in future experimental settings. From the lens of control and decision-making, a few biological systems relevant to chemotherapy, immunotherapy, and epidemics are considered in this work. Models are analyzed numerically and analytically in order to enhance the outcome of the system with a new control/decision. A new dosing plan for chemotherapy is identified and evaluated via in-silico experiments to optimally reduce the tumor volume at the end of the plan. The new dosing plan consists of two doses starting with a small dose at the beginning of the plan and an increased dose after a few weeks. Unlike traditional chemotherapy plans currently used, the proposed plan is neither a maximum tolerated dose, nor a metronomic/intermittent plan. Moreover, epidemic models under social distancing guidelines are studied. Considering a single interval social distancing based on the start time and the duration of the social distancing shows a linear relationship between optimal timing of the social distancing. Models analyzed in this work are generic and applicable to wide a range of applications.

## **Chapter 1**

## **Background**

The goal of scientific research is to advance knowledge that does not exist in the literature. Research process starts with a specific question and proposing a hypothesis to answer it. Hypotheses are formed to come up with a solution to an unmet need, or in order to have a better understanding of a phenamena. The next step is testing the proposed hypothesis, which can be done in two ways. Finding an available data set based on previous experiments which can be used to evaluate the newly generated hypothesis, or disigning a new experiment that can generate sufficient data for evaluating the hypothesis.

An in depth understanding of the scientific subject is necessary to come up with a new hypothesis or a new experiment design. Models are usefull in providing a simpler representation of a realworld phenamena, to have a better understanding and easy to test envonriment for creativity. In architecture, models are physical or computational 3D representation of a proposed building design to increase the construction speed and make the planning easier. In computing, emulators are hardware or software models the enable one computer to acts like another system. In biology, animal models are frequently used to create a realistic environment for biological experiments such as, immune cell and tumor, pharmacokinetics of a drug, or disease progression. In dynamic systems, mathematical models can be defined with Ordinary Differential Equation (ODE) to represent a mechanistic representation of the system. Mathematical models can be also defined in numerical formats such as, agent based models, and artificial neural networks. The creation of scientific fields like theoretical biology, math biology, systems biology, computational biology, or systems and computational medicine are all based on using mathematical models in theoretical studies of biological systems. These studeis are interdisciplinary and require collaboration of people with different backgrounds. A simple analogy is that, understanding biology requires chemistry, understanding chemistry requires physics, and

#### CHAPTER 1. BACKGROUND

understanding physics requires math.

The objective is to perform numerical and analytical analysis from the control theory perspective. The techniques used in control theory, which deals with the control of dynamical systems in engineered processes and machines, can be applied to mathematical models of biological systems. Medicine can be thought as a control input for a biological system like an animal or a human. Also, considering the spread of an epidemic disease in a society as a biological system, Nonpharmaceutical Intervention (NPI) like social distancing can be thought as a control input. The following section is about the role of mathematical modeling in theory and practice. A couple of well-known examples are discussed to illustrate the importance of modeling in scientific research. The focus and organisation of this study is discussed at the end of this chapter.

#### 1.1 Theory and practice

Theory and practice are the two fundamental tools in scientific research. Classic biology has been thought as a practical science. With a great increase of quantitive experiments in biological systems over the past decates, more theoretical studies are possible in biology.

Figure 2.5a presents a visual representation of the connection between theory and practice. In theory, models that are based on the existing knowledge (data) are being used in order to come up with new hypotheses. Some of the newly generated hypothesis can be tested by using the existing data, which is common in data science. Other hypotheses require a new data set being generated for testing. In practice a hypothesis that is formed based on the existing knowledge, have to be tested with a new experiment design. In the following, two of the most important scientific discoveries as an example of the presented analogy between theory and practice.

#### 1.1.1 Gravitational waves

By considering models as a framework to generalize the previous experimental data. One could have the power of predicting the results of experiments that has not existed before. The discovery of gravitational waves is one the most important examples for models that could predict above and beyond the present data.

Gravity has been the most basic and mysterious force in physics. Understanding gravity is one of the examples that started with theory and mathematical models. Einstein predicted gravitational waves in 1937 [1] based on his theory of relativity. But the universe's gravitational

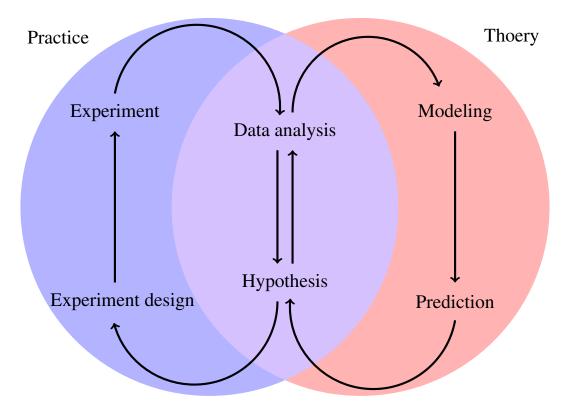


Figure 1.1: Theory and practice in research: In practice, the left circle, the objective is to come up with a new experiment design that can produce a data set for answering a scientific hypothesis. In theory, the right circle, the objective is to use a model that *reasonably* represents the existing data to come up with new predictions and hypotheses. In data science, the objective is to come up with new hypotheses that can be answered with the existing data sets, which is becoming more popular.

#### CHAPTER 1. BACKGROUND

waves have not been detected until 2015, when a large group of researchers used Laser Interferometer Gravitational-Wave Observatory (LIGO), and they received the 2017 Nobel prise in physics.

#### 1.1.2 Genetic heredity

A scientific descovery without a proper model is missing a key feature. Genetic heredity is one of the most imporant examples for this scenario. Hypothesis could be frequently made from the data, but whether the hypothesis is true or not requires regorious analysis. Statistical analysis, that are based on statistical models, are frequently used in data science to answer hypothetical questions from the data.

Mendel used pea plants for cross-breeding experiments to discover the fundamental laws of genetic inheritance [2]. The discovery of the law of segregation, the law of indepdents assortment, and the law of dominance took him eight years, when he grew over 10,000 pea plants to track their genetic heredity. Mendel's dicovery was not widely accepted in scientific communities until Fisher pushlished a statistical analysis of Mendel's data [3].

#### 1.2 Focus of the dissertation

Trial and error has been the fundamental method in practice. Trial comes from the Anglo-French trier meaning "to try", and error means "a mistake". The procedue of trial and error strats by testing a hypothesis that might pass or fail, and iterating over modified versions of the starting hypothesis until it gets to a desired solution. The focus of this work is to utalize mathematical models in order to speed up the trail and error process. The number of possible experiment designs are often at a combinatorial scale, and mathematical models are necessary to bring more insight into the problem to optimize the number of tries.

Most achievements of biotechnology in pharmaceutical industry on *platform* thinking. *platform* is a machine that could automatically repeat exeriments with the desired inputs. *Platforms* are automated systems that enable scientist to make new discoveries with more depth, and speed. In other words, if the left hand side of Figure 2.5a (practice) is automated then scientist could spend more time on biology, the right hand side of Figure 2.5a (theory), to deepen their understanding to make new discoveries. The focus of this dissertation is the theoretical aspect of biological discoveries. For example, performing feasability study to answer hypothetical questions of the experimentalists, or optimization study to identify what changes of the input could optimize the objective.

#### 1.3 Organization of this work

Each of the following chapter in this work constits of using mathematical models for control of a biological systems. The contributions made in this work are both mathematical and computational based on the very specific applications. Each chapter is written independently. While, the models used here are considered to be generic and applicable to applications outside the focus of each study. The reader is encouraged to consider specific chapters of their interest.

Chapter 2 is based on a dynamic model of traslation process, Ribosome Flow Model (RFM). This project started by a question from one of the experimentalist, who thought it could be possible to change the inflow/outflow rates of ribosomes experimentally, and asked if the mRNA translation speed can be increased by using a periodic input. Early numerical results of the model was not in favor of periodic inputs. Meanwhile, theoretically it become an interesting tast to prove that constant inputs are always better for such a system. The rest of this dissertation is less theoretical. Chapter 4 discusses social distancing in compartmental epidemic models. Chapter 3 is dedicated to bispecific T-cell engagers.

## **Chapter 2**

### **Periodic Flow of Ribosomes**

This chapter is based on a compartmental model for ribosome flow during RNA translation called the Ribosome Flow Model (RFM). This model includes a set of positive transition rates that control the flow from every site to the consecutive site. It has been shown that when these rates are time-varying and jointly T-periodic every solution of the RFM converges to a unique periodic solution with period T. In other words, the RFM entrains to the periodic excitation. In particular, the protein production rate converges to a unique T-periodic pattern. From a biological point of view, one may argue that the average of the periodic production rate, and not the instantaneous rate, is the relevant quantity. The problem that this chapter investigates can be roughly stated as: can periodic rates yield a higher average production rate than constant rates in RFM? This question is regoriously formulated and shown via simulations, and rigorous analysis in one simple case, that the answer is no.

#### 2.1 Introduction

Transcription and translation are the two major steps of gene expression, that is, the transformation of the information encoded in the DNA into proteins. During translation complex molecular machines called ribosomes traverse the mRNA molecule, "read" it codon by codon, and generate the corresponding chain of amino-acids [4].

New imaging techniques [5–8] and empirical approaches [9–14] for studying gene expression provide unprecedented amounts of data on the dynamics of translation. This increases the need for mathematical and computational models for ribosome flow that can integrate, explain and make predictions based on this data (see the reviews [15–17]). Mechanistic models are particularly

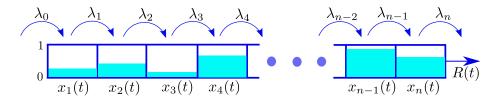


Figure 2.1: A visual representaion for Ribosome Flow Model (RFM).

important in biotechnology and synthetic biology, as they allow to predict the effect of various manipulations of the biological machinery [18, 19].

The RFM is a deterministic model for ribosome flow [20]. It can be derived via a dynamic mean-field approximation of a fundamental model from statistical physics called the Totally asymmetric Simple Exclusion Process (TASEP) [15, 21]. In TASEP particles hop randomly along a chain of ordered sites. A site can be either free or contain a single particle. Totally asymmetric means that the flow is unidirectional, and simple exclusion means that a particle can only hop into a free site. This models the fact that two particles cannot be in the same place at the same time. Note that this generates an indirect coupling between the particles. In particular, if a particle is delayed at a site for a long time then the particles behind it cannot move forward and thus a "traffic jam" may evolve.

The RFM is a compartmental model with n sites. The state-variable  $x_i(t)$ ,  $i=1,\ldots,n$ , describes the density of particles at site i at time t. This is normalized so that  $x_i(t)=0$  [ $x_i(t)=1$ ] means that site i is completely empty [full] at time t. The state-space is thus the closed unit cube  $[0,1]^n$ .

The dynamics is described by n first-order ODEs:

$$\dot{x}_1(t) = \lambda_0(1 - x_1(t)) - \lambda_1 x_1(t)(1 - x_2(t)), \tag{2.1a}$$

$$\dot{x}_k(t) = \lambda_{k-1} x_{k-1}(t) (1 - x_k(t)) - \lambda_k x_k(t) (1 - x_{k+1}(t)), \qquad 2 \le k \le n - 1, \tag{2.1b}$$

$$\dot{x}_n(t) = \lambda_{n-1} x_{n-1}(t)(1 - x_n(t)) - \lambda_n x_n(t). \tag{2.1c}$$

Here  $\lambda_i > 0$  is a parameter that describes the transition rate from site i to site i+1, with  $\lambda_0$  [ $\lambda_n$ ] called the entry [exit] rate. Eq. (2.1) can be explained as follows. The flow from site k to site k+1 is given by  $\lambda_k x_k (1-x_{k+1})$ , i.e. it increases when site k becomes fuller and decreases when site k+1 becomes fuller. This is a "soft" version of simple exclusion. The production rate at time t is the rate of ribosomes exiting site n, that is,  $R(t) := \lambda_n x_n(t)$ . Figure 2.1 is a visual representation of RFM.

In the context of mRNA translation, the  $\lambda_i$ 's depend on various biomechanical properties for example the abundance of tRNA molecules that deliver the amino-acids to the ribosomes. A

recent paper suggests that cells vary their tRNA abundance in order to control the translation rate [22].

Note that if  $\lambda_k$  is small for some k then the flow from site k to site k+1 will be small, so site k fills up, that is  $x_k(t)$  will be close to one for all t sufficiently large. Consequently, the flow  $\lambda_{k-1}x_{k-1}(1-x_k)$  from site k-1 to site k will become small and then site k-1 fills up. In this way, a traffic jam may evolve behind a "bottleneck" site. The implications of such traffic jams in various biological transport processes is recently attracting considerable interest (see, e.g. [23, 24]).

It has been shown [25] that there exists a unique  $e = e(\lambda_0, \dots, \lambda_n) \in (0, 1)^n$  such that any solution of the RFM emanating from the unit cube converges to e. Thus, the system is globally asymptotically stable. In particular, the production rate converges to the steady-state value

$$R := \lambda_n e_n. \tag{2.2}$$

Ref. [26] derived a spectral representation for the steady-state density e and production rate R. Given the RFM, define the  $(n+2) \times (n+2)$  tridiagonal matrix:

$$B := \begin{bmatrix} 0 & \lambda_0^{-1/2} & 0 & 0 & \dots & 0 & 0 \\ \lambda_0^{-1/2} & 0 & \lambda_1^{-1/2} & 0 & \dots & 0 & 0 \\ 0 & \lambda_1^{-1/2} & 0 & \lambda_2^{-1/2} & \dots & 0 & 0 \\ & & & \vdots & & & \\ 0 & 0 & 0 & \dots & \lambda_{n-1}^{-1/2} & 0 & \lambda_n^{-1/2} \\ 0 & 0 & 0 & \dots & 0 & \lambda_n^{-1/2} & 0 \end{bmatrix}. \tag{2.3}$$

Note that B is (componentwise) nonnegative and irreducible. Let  $\sigma > 0$  [ $\zeta \in \mathbb{R}^{n+2}_{>0}$ ] denote the Perron root [Perron vector] of B (see e.g. [27]). Then

$$R = \sigma^{-2} \text{ and } e_i = \frac{\zeta_{i+2}}{\lambda_i^{1/2} \sigma \zeta_{i+1}}, \ i = 1, \dots, n.$$
 (2.4)

In other words, the steady-state values can be determined without any numerical simulations of the dynamics but rather using (efficient and numerically stable) algorithms for determining the Perron root and vector of tridiagonal matrices. Note that it follows from (2.4) that

$$R(c\lambda_0, \dots, c\lambda_n) = cR(\lambda_0, \dots, \lambda_n), \quad \text{for all } c > 0,$$
 (2.5)

that is, the steady-state production rate is positively homogeneous of degree one.

#### **2.1.1** Example

Consider the RFM with all the rates equal to one. Then B is a tridiagonal Toeplitz matrix and it is well-known (see e.g. [28]) that its eigenvalues are

$$2\cos(\frac{k\pi}{n+3}), \quad k = 1, \dots, n+2,$$
(2.6)

so the Perron root is  $\sigma = 2\cos(\frac{\pi}{n+3})$ . The corresponding Perron vector is

$$\zeta = \left[ \sin\left(\frac{\pi}{n+3}\right) \quad \sin\left(\frac{2\pi}{n+3}\right) \quad \dots \quad \sin\left(\frac{(n+2)\pi}{n+3}\right) \right]^{T}. \tag{2.7}$$

Thus, in this case (2.4) gives

$$R = \frac{1}{4} \left(\cos(\frac{\pi}{n+3})\right)^{-2} \tag{2.8}$$

and

$$e_i = \frac{\zeta_{i+2}}{\sigma \zeta_{i+1}} \tag{2.9a}$$

$$= \frac{\sin(\frac{(i+2)\pi}{n+3})}{2\cos(\frac{\pi}{n+3})\sin(\frac{(i+1)\pi}{n+3})}$$
(2.9b)

for all  $i=1,\ldots,n$ . For example, in the one-dimensional case, i.e.  $\dot{x}_1=1-2x_1$  it is clear that the equilibrium point is e=1/2, so R=1/2, whereas (2.8) yields

$$R = \frac{1}{4}(\cos(\frac{\pi}{4}))^{-2} = 1/2,$$
(2.10)

and (2.9a) gives

$$e_1 = \frac{\sin(\frac{3\pi}{4})}{2\cos(\frac{\pi}{4})\sin(\frac{2\pi}{4})} = 1/2.$$
 (2.11)

#### 2.1.2 Periodic excitation

Biological organisms are exposed to periodic excitations like the 24h solar day and the periodic cell-cycle division process. Proper functioning often requires entrainment to such excitations i.e. internal processes must operate in a periodic pattern with the same period as the excitation. An example is the sleep-wake cycle that entrains to the 24h day.

Ref. [29] studied the RFM with positive time-varying rates that are jointly T-periodic, and proved that every state-variable  $x_i(t)$  converges to a periodic solution with period T. In other words, the RFM entrains. The proof is based on the fact that the RFM is an (almost) contractive system [30,

31]. However, this provides no information on the attractive periodic solution (except for its period). Obtaining such information is a difficult problem (see [32] and the references therein).

Since any set of jointly periodic rates induces a periodic solution, a natural question is: can periodic rates yield a higher production rate than constant rates? In this paper, we formulate this question rigorously, and show that it can be cast as an optimal control problem.

#### 2.1.3 Bottleneck entrance

In an analogous point of view, the RFM can be thought as a "bottleneck entrance". And generalized to more applications like traffic systems, and scheduling at security checks with a cascade of an arbitrary Hurwitz positive linear system. The cascade system etrains i.e. in response to a T-periodic inflow every solution converges to a unique T-periodic solution of the system. And, the objective would be to choose a periodic inflow rate with a given mean value that maximizes the average outflow rate of the system when maximizing the throughput is crucial.

The occupancy at time t in such applications can be modeled by the normalized state-variable  $x(t) \in [0,1]$ . In traffic systems, x(t) can be interpreted as the number of vehicles relative to the maximum capacity of a highway segment. For the security check, it is the number of passengers at a security gate relative to its capacity. In biological transport models discussed in the previous sections, x(t) is interpreted as the probability that a biological "machine" (e.g. ribosome, motor protein) is bound to a specific segment of the "trail" it is traversing (e.g. mRNA molecule, filament) at time t.

The output in such systems is a nonnegative outflow which can be interpreted as the rate of cars exiting the highway for the traffic system, or passengers leaving the gate for the security check. The inflow rates are often periodic, such as those controlled by traffic light signals, or periodic flight schedules. Proper functioning often requires *entrainment* to such excitations i.e. internal processes must operate in a periodic pattern with the same period as the excitation [33]. In this case, in response to a T-periodic inflow the outflow converges to a T-periodic pattern, and the *throughput* is then defined as the ratio of the average outflow relative to the average inflow over the period T.

As a general model for studying such applications is the cascade of two systems shown in Fig. 2.2. The first block is called the *bottleneck* and is given by:

$$\dot{x}(t) = \sigma(t)(1 - x(t)) - \lambda x(t), \tag{2.12a}$$

$$w(t) = \lambda x(t), \tag{2.12b}$$

$$\begin{array}{c|c} \sigma(t) & \dot{x} = \sigma(t)(1-x) - \lambda x \\ \hline w = \lambda x \\ \hline \end{array} \begin{array}{c|c} \dot{x} = Az + bw \\ \hline y = c^T z \\ \hline \end{array}$$

Figure 2.2: Cascade system: the bottleneck is feeding a positive linear system.

where  $\sigma(t) > 0$  is the inflow rate at time  $t, x(t) \in [0, 1]$  is the occupancy of the bottleneck, and  $\lambda > 0$  controls the output flow w(t). The rate of change of the occupancy is proportional to the inflow rate  $\sigma(t)$  and the *vacancy* 1 - x(t), that is, as the occupancy increases the effective entry rate decreases.

A standard notation in this study. Vectors [matrices] are denoted by small [capital] letters. For a vector x, x' denotes the transpose of x. To follow the standard practice of identifying any two measurable functions that are identical except perhaps on a set of measure zero.

Assuming that the inflow is periodic with period  $T \geq 0$ , i.e.  $\sigma(t+T) = \sigma(t)$  for all  $t \geq 0$ . The occupancy x(t) (and thus also w(t)) entrains, as the system is contractive [34, 35]. In other words, for any initial condition  $x(0) \in [0,1]$  the solution x(t) converges to a unique T-periodic solution denoted  $x_{\sigma}$  and thus w converges to a T-periodic solution  $w_{\sigma}$ .

The outflow of the bottleneck is the input into a Hurwitz positive linear system:

$$\dot{z} = Az + bw, \tag{2.13a}$$

$$y = c^T z, (2.13b)$$

where  $A \in \mathbb{R}^{n \times n}$  is Hurwitz and Metzler and  $b, c \in \mathbb{R}^n_+$  (see Figure 2.2). It is clear that for a T-periodic  $\sigma(t)$ , all trajectories of the cascade converge to a unique trajectory  $(x_{\sigma}(t), z_{\sigma}(t))$  with  $x_{\sigma}(t) = x_{\sigma}(t+T)$  and  $z_{\sigma}(t) = z_{\sigma}(t+T)$ .

The objective for these applications is to compare the average (over a period) of  $y_{\sigma}(t)$  for various T-periodic inflows. To make a meaningful comparison, consider inflows that have a fixed mean  $\bar{\sigma}>0$ , i.e

$$\frac{1}{T} \int_0^T \sigma(t) \, \mathrm{d}t = \bar{\sigma}. \tag{2.14}$$

The objective is maximize the gain of the system from  $\sigma$  to y, i.e to maximize  $\int_0^T y_{\sigma}(t) dt$  for inputs with mean  $\bar{\sigma}$ .

The trivial periodic inflow rate is the constant rate  $\sigma(t) \equiv \bar{\sigma}$ . To compare the outflow for this constant inflow with that obtained for an inflow that switches between two values  $\sigma_1$  and  $\sigma_2$  such that  $\sigma_2 > \bar{\sigma} > \sigma_1 > 0$ . In other words,  $\sigma(t) \in {\sigma_1, \sigma_2}$  is periodic and satisfies (2.14).

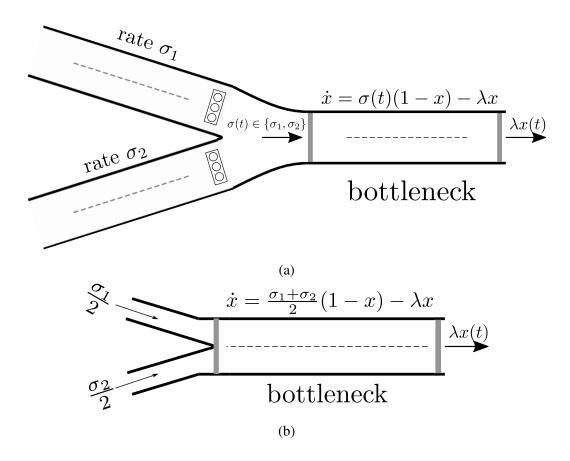


Figure 2.3: Traffic system application illustrating the two strategies. Here  $x(t) \in [0, 1]$  denotes the occupancy of the bottleneck at time t. (a) The inflow rate switches via periodically-varying traffic lights between two flows with rates  $\sigma_1, \sigma_2$ . At each time, either vehicles in the upper lane or vehicles in the lower lane can enter the bottleneck, but not both. (b) The double lane of each flow is restricted to a single lane and connected directly to the corresponding lane in the bottleneck.

For the application in traffic system depicted in Figure 2.3, there are two flows of vehicles with different rates  $\sigma_1, \sigma_2$  (e.g., cars and trucks) each moving in a separate road and joining into a two-lane highway. This can be done in two ways. The first is to place traffic lights at the end of each road, and switch between them before entering the highway as in Figure 2.3(a). The periodic traffic light signal  $\sigma(t)$  switches between the two flows, hence  $\sigma(t) \in \{\sigma_1, \sigma_2\}$ . The second strategy is to have each road constricted to a single lane, and then each joining the corresponding lane in the highway as in Figure 2.3(b). Hence, the inflow rate is constant and equal to  $(\sigma_1 + \sigma_2)/2$ . In both cases, the occupancy x(t) of the highway is modeled by (2.12a). For a proper comparison,  $\frac{1}{T} \int_0^T \sigma(t) \, \mathrm{d}t = (\sigma_1 + \sigma_2)/2$  as discussed before.

#### 2.1.4 Problem Formulation

For any T-periodic function f, with T>0, let  $\bar f:=\frac1T\int_0^T f(t)\,\mathrm{d} t$ , that is, the average of f over a period. Pick a set of rates  $\lambda_i(t),\,i=1,\ldots,n$ , that are jointly T-periodic (note that a constant rate is T-periodic for any T). This induces a unique T-periodic trajectory  $\gamma(t)$  of the RFM and thus a unique T-periodic production rate  $R_T(t):=\lambda_n(t)\gamma_n(t)$  [29]. The average production rate is thus  $\overline{R_T}$ . Consider an RFM with constant rates  $\overline{\lambda_i},\,i=1,\ldots,n$ . Recall that every trajectory converges to a unique steady-state e and thus to a production rate  $R:=\overline{\lambda_n}e_n$ .

The question of interest in this study is: what is the relation between  $\overline{R_T}$  and R? Note that this is a "fair" comparison as we replace every time-varying rate by its average value.

More generally, we can take a set of admissible rates  $S_{a,T}$  that are all jointly T-periodic and satisfy  $\overline{\lambda_i} = a_i$ . Recall  $\sup_{S_{a,T}} \{\overline{R_T}/R\}$ , where the sup is with respect to all the (non-trivial) rates in  $S_{a,T}$ , the *periodic gain* of the RFM over  $S_{a,T}$ . One can argue that the average production rate over a period, rather than the instantaneous value, is the biologically relevant quantity. Then a periodic gain larger than one implies that we can "do better" using periodic rates. A periodic gain one implies that we do not "loose" anything with respect to the constant rates  $\lambda_i(t) \equiv a_i$ . A periodic gain smaller than one implies that for any (non-trivial) periodic rate the average production rate is lower than the one obtained for constant rates. This implies that entrainment always incurs a cost, as the production rate for constant rates is higher.

#### 2.1.5 Structure of this chapter

The remainder of this paper is organized as follows. Section 2.2 describes some simulation results for the general RFM. Section 2.3 shows that the problem of finding the periodic gain can be cast as an optimal control problem. This implies that the problem can be addressed using known and powerful tools from optimal control theory [36–38]. By applying Pontryagin Maximum Principle (PMP) to analyze a particular case, namely, a one-dimensional RFM with a constant  $\lambda_1$  and a time-varying and periodic  $\lambda_0(t)$ .

#### 2.2 Numerical simulations

To gain a wider perspective, consider the case of a Single-Input Single-Output (SISO) asymptotically stable Linear Time-Inveriant (LTI) system with input [output] u(t) [y(t)] and transfer

function G(s). Fix  $\omega, a > 0$ . Suppose that the set of admissible inputs is

$${a + b\sin(\omega t) : b \in \mathbb{R}}.$$

Note that every input here is T-periodic with  $T:=2\pi/\omega$ , and that  $\overline{u}=a$ . It is well-known that for  $u(t)=a+b\sin(\omega t)$  the output converges to the T-periodic function  $y_T(t):=|G(0)|a+|G(j\omega)|b\sin(\omega t+\angle G(j\omega))$ , where  $j:=\sqrt{-1}$ , so  $\overline{y_T}=|G(0)|a$ . On the other-hand, if we replace u(t) by a constant input with value  $\overline{u}=a$  then the output converges to |G(0)|a. Thus, the periodic gain for this set of admissible inputs is one and by superposition it is one for any set of admissible T-periodic inputs with average a.

Of course, for nonlinear systems, like the RFM, the periodic gain may be different than one. The next example demonstrates this.

#### **2.2.1 Example**

Consider the scalar system

$$\dot{x}(t) = 1 - x(t)u(t). \tag{2.15}$$

For

$$u(t) = 1 + (1/2)\cos(\omega t),$$
 (2.16)

with  $\omega > 0$ , the solution is

$$x(t) = \exp(-t - \frac{\sin(\omega t)}{2\omega})(x(0) + \phi(t)), \tag{2.17}$$

where  $\phi(t):=\int_0^t \exp(s+\frac{\sin(\omega s)}{2\omega})\,\mathrm{d}s.$  In particular, for  $T:=2\pi/\omega,$ 

$$x(T) = \exp(-T)(x(0) + \phi(T)). \tag{2.18}$$

Now determine an initial condition x(0) = c for which the solution is T-periodic, that is,

$$c = \exp(-T)(c + \phi(T)), \tag{2.19}$$

so

$$c = \frac{\exp(-T)\phi(T)}{1 - \exp(-T)}.$$
 (2.20)

Thus, the periodic solution is  $x_T(t) := \exp(-t - \frac{\sin(\omega t)}{2\omega})(c + \phi(t))$ . It is not difficult to show that this solution is attractive.

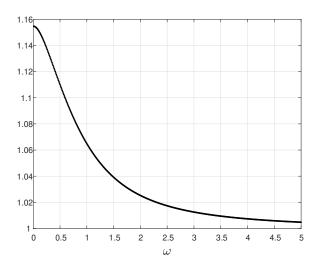


Figure 2.4: Periodic gain in Example 2.2.1 as a function of  $\omega$ .

On the other-hand, for a constant control with value  $\overline{u} = \frac{1}{T} \int_0^T u(s) \, \mathrm{d}s = 1$ , the solution of (2.15) converges to the steady-state 1 and thus the periodic gain for the control (2.16) is  $\overline{x_T} = \frac{1}{T} \int_0^T x_T(t) \, \mathrm{d}t$ . Fig. 2.4 depicts  $\overline{x_T}$  as a function of  $\omega$ . It may be seen that the periodic gain is always larger than 1, and that it approaches 1 as  $\omega \to \infty$ .

#### 2.2.2 Harmonic functions

The RFM where every rate is a sum of m harmonic functions with random coefficients. More precisely, we generated a matrix of random entries  $P \in \mathbb{R}^{(n+1)\times(2m)}$  and then set

$$\lambda_i(t) = 1 + \sum_{k=1}^{m} (p_{i,2k-1}\sin(k\omega t) + p_{i,2k}\cos(k\omega t)), \qquad i = 0,\dots, n.$$
 (2.21)

Note that this guarantees that the  $\lambda_i$ 's are jointly T-periodic for  $T=2\pi/\omega$  and that  $\overline{\lambda}_i=1$  for all i. The entries of P are generated randomly with a uniform distribution over [-1/(2m),1/(2m)], so that  $\lambda_i(t)\geq 0$  for all i and all t.

The RFM with n=1 is simulated first. Since  $\overline{\lambda_i}=1$  for i=0,1, and example 2.2.1, it can be concluded that R=1/2. Fig. 2.5a depicts a histogram of the average steady-state flow  $\overline{R_T}$  for m=3 and 10,000 random simulations. It may be seen that  $\overline{R_T}$  is always smaller than 1/2. Thus, the constant rates yield the maximal production rate.

To explain this, consider the case where  $\lambda_1=1$  and  $\lambda_0(t)=1+\sin(\omega t)$ . Let us compare this to the case where  $\lambda_1=1$  and  $\lambda_0=1$ . At times t such that  $\sin(wt)=-1$ , there is less flow

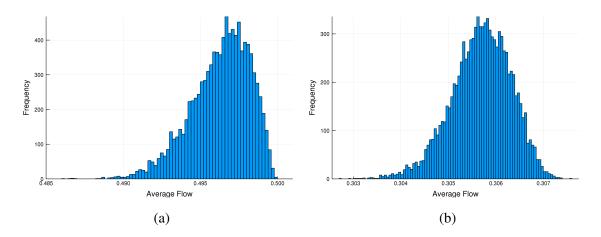


Figure 2.5: Numerical simulations: (a) A histogram of  $\overline{R_T}$  values in the one-dimensional RFM with random periodic  $\lambda_0(t)$  and  $\lambda_1(t)$ . (b) A histogram of  $\overline{R_T}$  values in an RFM with n=4 and periodic rates  $\lambda_i(t)$ ,  $i=0,\ldots,4$ .

because  $\lambda_0(t)=0$ . At times t such that  $\sin(\omega t)=1$ , there is more flow because  $\lambda_0(t)=2$ , but then  $\lambda_1$  becomes a bottleneck rate and slows down the flow, and thus on average we don't gain enough flow to compensate for what is lost. This might be called the "casino effect": on average, the gains are not enough to compensate for the losses.

Consider now an RFM with n=4 and constant rates set to one. By (2.8),

$$R = \frac{1}{4}(\cos(\pi/7))^{-2} \approx 0.307979. \tag{2.22}$$

Fig. 2.5b depicts a histogram representation of  $\overline{R_T}$  calculated over 10,000 simulations of an RFM with random periodic rates  $\lambda_0(t), \ldots, \lambda_4(t)$ . It may be seen that  $\overline{R_T}$  is smaller than the value in (2.22), so again the constant rates are those that maximize the production rate.

### 2.3 Optimal periodic control

The next goal is to pose the problem of determining the RFM periodic gain as an optimal control problem. The equations of the RFM can be augmented with an additional state-variable as

follows

$$\dot{z}_1 = \lambda_0 (1 - z_1) - \lambda_1 z_1 (1 - z_2), \tag{2.23a}$$

$$\dot{z}_k = \lambda_{k-1} z_{k-1} (1 - z_k) - \lambda_k z_k (1 - z_{k+1}), \qquad 2 \le k \le n - 1, \tag{2.23b}$$

$$\dot{z}_n = \lambda_{n-1} z_{n-1} (1 - z_n) - \lambda_n z_n, \tag{2.23c}$$

$$\dot{z}_{n+1} = \lambda_n z_n, \quad z_{n+1}(0) = 0. \tag{2.23d}$$

Thus,  $z(t) = \int_0^t R(\tau) d\tau$ . Pick T > 0 and  $a_1, \ldots, a_n > 0$ , and let  $S_{a,T}$  denote the set of measurable functions  $\lambda_i : [0,T] \to \mathbb{R}_+$  such that  $\overline{\lambda_i} = a_i, i = 0, \ldots, n$ .

By applying the spectral representation to determine the steady-state production rate R when  $\lambda_i(t) \equiv a_i$  for all i. Thus, determining the periodic gain is equivalent to solving the following optimization problem.

**Problem 1.** Maximize  $\frac{1}{T}z_{n+1}(T)$  over the set of admissible rates  $S_{a,T}$  with the boundary condition  $z_i(0) = z_i(T) \in (0,1)$  for  $i = 1, \ldots, n$ .

The last condition guarantees that we are maximizing the production rate along the (unique) periodic trajectory. This optimal control problem can be addressed using known tools from optimal control theory [36–38]. This special case can be demonstrated as follows.

#### **2.3.1** The case n = 1

Pick  $T,a_0>0$ , and consider the problem of computing the periodic gain of the onedimensional RFM with a constant  $\lambda_1>0$  and a time-varying  $\lambda_0:[0,T]\to\mathbb{R}_+$  with  $\overline{\lambda_0}=a_0$ .

Consider first the special case where  $\lambda_0(t)$  is constant. Then clearly  $\lambda_0(t) \equiv a_0$ , and thus

$$\dot{x}_1 = a_0(1 - x_1) - \lambda_1 x_1. \tag{2.24}$$

The steady-state of this equation is  $e_1 = \frac{a_0}{a_0 + \lambda_1}$ , so  $\overline{R} = \frac{\lambda_1 a_0}{a_0 + \lambda_1}$ .

To study the case where  $\lambda_0(t)$  is not constant, it is useful to incorporate the constraint  $\overline{\lambda_0}=a_0$  into the dynamics. Thus, the following system is considered.

$$\dot{x}_1(t) = \lambda_0(t)(1 - x_1(t)) - \lambda_1 x_1(t), \tag{2.25a}$$

$$\dot{x}_2(t) = \lambda_0(t),\tag{2.25b}$$

with the boundary conditions

$$x_1(T) = x_1(0), \ x_2(0) = 0, \ x_2(T) = Ta_0.$$
 (2.26)

Fix  $L \geq 2a_0$ . Determining the periodic gain is equivalent to solving the following problem.

**Problem 2.** Find  $\lambda_0:[0,T]\to[0,L]$  that maximizes the cost functional

$$J := \frac{1}{T} \int_0^T \lambda_1 x_1(t) \, \mathrm{d}t,\tag{2.27}$$

subject to the dynamics (2.25) and the boundary conditions (2.26).

The added bound on the size of  $\lambda_0(t)$  is needed because the presented solution in this study is using the PMP.

Note that the model (2.25) can rewritten as a bilinear control system.

$$\dot{x} = f(x) + g(x)u, \tag{2.28}$$

where u represents  $\lambda_0$ ,  $f(x) := \begin{bmatrix} -\lambda_1 x_1 & 0 \end{bmatrix}'$ , and  $g(x) := \begin{bmatrix} 1 - x_1 & 1 \end{bmatrix}'$ . Thus, Problem 2 is a nonlinear optimal control problem (for other control problems for the RFM, see [39]).

The main result of this study can be stated as:

**Theorem 1.** For any  $L \ge 2a_0$  the unique solution of Problem 2 is the constant rate:

$$\lambda_0^*(t) \equiv a_0, \tag{2.29}$$

and the corresponding optimal cost is:

$$J^* = \frac{\lambda_1 a_0}{\lambda_1 + a_0}. (2.30)$$

Hence, the steady-state average flow of the system cannot be improved by using a periodic rate.

The proof of Theorem 1 is based on applying the PMP to analyze the structure of optimal controls.

#### 2.3.2 Pontryagin's maximum principle for periodic trajectories

We apply the PMP to Problem 2. The statement of the PMP in our case is standard, except perhaps for the constraint that forces maximization over the periodic solution, i.e.  $x_1(0) = x_1(T)$ .

Define the Hamiltonian

$$\mathcal{H}(u, x, p, p_0) := p'(f(x) + g(x)u) + \frac{1}{T}p_0\lambda_1 x_1$$
 (2.31a)

$$= (-p_1\lambda_1 + p_0\frac{1}{T}\lambda_1)x_1 + (p_1(1-x_1) + p_2)u, \tag{2.31b}$$

where  $p(t) := \begin{bmatrix} p_1(t) & p_2(t) \end{bmatrix}'$  is the adjoint, and  $p_0 \ge 0$  is called the abnormal multiplier. Note that we can scale the Hamiltonian by scaling u and  $\lambda_1$ . Thus, from here on we assume without loss of generality that  $\lambda_1 = 1$ .

**Proposition 2** (PMP). Let  $u^*(t): [0,T] \to [0,L]$  be an optimal control for Problem 2. Let  $x^*: [0,T] \to ([0,1] \times \mathbb{R}_+)$  be the corresponding optimal trajectory. Let  $p_0^*:=T$ . There exists a function  $p^*: [0,T] \to \mathbb{R}^2 \setminus \{0\}$  such that:

1. The functions  $x^*(t)$  and  $p^*(t)$  satisfy:

$$\dot{x}^* = \frac{\partial \mathcal{H}}{\partial p}(u^*, x^*, p^*, p_0^*), \tag{2.32a}$$

$$\dot{p}^* = -\frac{\partial \mathcal{H}}{\partial x}(u^*, x^*, p^*, p_0^*); \tag{2.32b}$$

2. The control  $u^*(t)$  satisfies

$$\mathcal{H}(s, x^*(t), p^*(t), p_0^*) \le \mathcal{H}(u^*(t), x^*(t), p^*(t), p_0^*) \tag{2.33}$$

for all  $s \in [0, L]$  and almost every (a.e.)  $t \in [0, T]$ ;

3. The adjoint satisfies the transversality condition:

$$p_1^*(0) = p_1^*(T). (2.34)$$

A few remarks will be discussed before proving Proposition 2. First, note that (2.32a) yields

$$\dot{p}_1^* = (1+u)p_1^* - 1, \quad \dot{p}_2^* = 0.$$
 (2.35)

so  $p_2^*(t) \equiv p_2^*(0)$ . Second, define the switching function  $\varphi^*: [0,T] \to \mathbb{R}$  by

$$\varphi^*(t) := (p^*(t))' g(x^*(t)) \tag{2.36a}$$

$$= p_1^*(t)(1 - x_1^*(t)) + p_2^*(0). (2.36b)$$

Note that  $\varphi^*(t)$  is absolutely continuous. Then (2.33) implies that

$$u^{*}(t) = \begin{cases} L, & \varphi^{*}(t) > 0, \\ 0, & \varphi^{*}(t) < 0. \end{cases}$$
 (2.37)

A calculation yields

$$\dot{\varphi}^* = \dot{p}_1^* (1 - x_1^*) - p_1^* \dot{x}_1^* \tag{2.38a}$$

$$= p_1^* - 1 + x_1^*, \tag{2.38b}$$

$$\ddot{\varphi}^* = \dot{p}_1^* + \dot{x}_1^* \tag{2.38c}$$

$$= (1 - x_1^* + p_1^*)u - 1 - x_1^* + p_1^*. (2.38d)$$

Note that this implies that  $\dot{\varphi}^*$  is absolutely continuous, so  $\varphi^* \in C^1$ .

*Proof of Proposition 2.* Most of the statements here are the standard PMP. It is only necessary to prove the transversality condition (2.34), and that  $p_0^* \neq 0$ .

Pick  $S \subseteq \mathbb{R}^4$ , and suppose that the state must satisfy the constraint  $\begin{bmatrix} x(0) & x(T) \end{bmatrix}' \in S$ . Then the transversality condition [37] is

$$\begin{bmatrix} p(0) \\ -p(T) \end{bmatrix} \perp \mathcal{T}_{\begin{bmatrix} x(0) \\ x(T) \end{bmatrix}} S, \tag{2.39}$$

where  $\mathcal{T}_zS$  is the tangent space of S at z. In this case,  $S = \{z \in \mathbb{R}^4 | z_1 - z_3 = 0, z_2 = 0, z_4 = Ta_0\}$ . Hence,  $T_zS = \text{span}\{[1,0,1,0]'\}$ . Therefore, it is necessary that  $p_1^*(0) = p_1^*(T)$ .

Next we show that the abnormal multiplier is not zero. Assume that  $p_0^*=0$ . Then (2.32a) yields

$$\dot{p}_1^* = (1 + u^*)p_1^*. \tag{2.40}$$

Thus,  $p_1^*(t) \ge \exp(t)p_1^*(0)$  for all  $t \ge 0$ . If  $p_1^*(0) \ne 0$  then this contradicts (2.34), so we conclude that  $p_1^*(0) = 0$  and thus  $p_1^*(t) \equiv 0$ . This implies that  $p_2^*(0) \ne 0$ , and thus (2.36a) and (2.37) imply that  $u^*(t)$  is constant. But in this case it is clear that  $u^*(t) \equiv a_0$ . It can be concluded that by assuming  $p_0^* \ne 0$ , and by scaling the result is  $p_0^* = T$ .

#### 2.3.3 The structure of an optimal control

Given an optimal control  $u^*$ , let

$$E_{\perp}^* := \{ t \in [0, T] : \varphi^*(t) > 0 \}, \tag{2.41a}$$

$$E_{-}^{*} := \{ t \in [0, T] : \varphi^{*}(t) < 0 \}, \tag{2.41b}$$

$$E_0^* := \{ t \in [0, T] : \varphi^*(t) = 0 \}. \tag{2.41c}$$

Note that all these sets are measurable.

The next result analyzes singular arcs. For a measurable set  $F\subseteq [0,T]$ , we use  $\mu(F)$  to denote the Lebesgue measure of F.

**Lemma 3.** Suppose that  $u^*$  is an optimal control such that  $\mu(E_0^*) > 0$ . Then there exists a unique  $c_0 \in (0, L]$  such that

$$u^*(t) \equiv c_0 \text{ for a.e. } t \in E_0^*,$$
 (2.42)

and

$$x_1^*(t) \equiv \frac{c_0}{1+c_0} \text{ for all } t \in E_0^*.$$
 (2.43)

*Proof.* Let  $E^* \subseteq E_0^*$  denote the set of accumulation points of  $E_0^*$ . Note that  $\mu(E^*) = \mu(E_0^*)$ , since  $E_0^* - E^*$  is the set of isolated points of  $E^*$  which is countable, and hence has measure zero. For  $t \in E^*$ , we have  $\varphi^*(t) = 0$ , so  $(\varphi^*(t))^{(k)} := \frac{d^k}{dt^k} \varphi^*(t) = 0$  for any integer  $k \ge 0$ .

The equation  $\varphi^*(t)=\dot{\varphi}^*(t)=0$  yields  $p_1^*(t)(1-x_1^*(t))\equiv -p_2^*(0)$ , and  $p_1^*(t)\equiv 1-x_1^*(t)$ . It can be concluded that

$$p_1^*(t) \equiv 1 - x_1^*(t) \equiv r, \tag{2.44}$$

where r is a constant. Since  $x^*(t) \in (0,1), r \in (0,1)$ . Hence,  $p_2^*(0) = -r^2 < 0$ .

Combining (2.44) with the fact that  $\ddot{\varphi}^*(t) = 0$  yields

$$u^*(t) \equiv c_0, \tag{2.45}$$

where  $c_0 := \frac{1-r}{r}$ . Note that since  $u^*(t) \leq L$ ,

$$r(1+L) \ge 1. (2.46)$$

Now (2.44) yields 
$$x_1^*(t) \equiv 1 - r = \frac{c_0}{1 + c_0}$$
.

Note that if r(1+L)=1 then on any singular arc we have  $u^*(t)=c_0=L$ . This case is "not interesting" as then we can identify the singular arc with a bang arc. Thus from here on the assumption is that

$$r(1+L) > 1. (2.47)$$

The notation B[S] is used to denote a bang [singular] arc. The bang arc can be either  $B_+$  (i.e.  $\varphi^*(t) > 0$  on the arc), or  $B_-$ . The next result considers the concatenation of singular and bang arcs.

**Proposition 4.** An optimal control  $u^*$  cannot contain a concatenation of arcs in the form SBS.

*Proof.* Suppose that  $u^*$  includes a concatenation SBS. It is already known that there exists a unique value r such that  $x_1^*(t) \equiv 1 - r$  and  $p_1^*(t) \equiv r$  on both singular arcs.

Suppose that  $B = B_-$ . Then  $\dot{x}_1^* = -x_1^*$  along the bang arc, so  $x_1^*(t)$  strictly decreases on  $B_-$ . But this is a contradiction, as  $x_1^*(t)$  must have the same value on both singular arcs.

Suppose now that  $B = B_+$ . Then

$$\dot{p}_1^* = (1+L)p_1^* - 1^* \tag{2.48}$$

along the bang arc. In particular, at the initial time  $\tau \in (0,T)$  of  $B_+$ ,

$$\dot{p}_1^*(\tau) = (1+L)r - 1^* \tag{2.49}$$

and (2.47) yields  $\dot{p}_1^*(\tau) > 0$ . Combining this with (2.48) implies that  $p_1^*(t)$  strictly increases on  $B_+$  and this is again a contradiction.

The next result analyzes optimal controls that include two consecutive bang arcs.

**Lemma 5.** An optimal control  $u^*$  cannot include any of the following concatenations:  $B_-B_+B_-$ ,  $B_-B_+S$ ,  $B_+B_-B_+$ , and  $B_+B_-S$ .

*Proof.* Suppose that  $u^*$  includes  $B_+B_-$ . Then there exists  $\tau \in (0,T)$  such that  $\varphi^*(t) > 0$  for  $t \in (\tau - \varepsilon, \tau)$ , and  $\varphi^*(t) < 0$  for  $t \in (\tau, \tau + \varepsilon)$ , with  $\varepsilon > 0$ . Hence  $\varphi^*(\tau) = 0$  and  $\dot{\varphi}^*(\tau) \leq 0$ . Combining this with (2.38a) yields

$$p_1^*(\tau) - 1 + x_1^*(\tau) \le 0. (2.50)$$

For any  $t \in (\tau, \tau + \varepsilon)$  it is true that  $u^*(t) = 0$ , so  $\dot{x}_1^*(t) = -x_1^*(t)$  and  $\dot{p}_1^*(t) = p_1^*(t) - 1$ . Thus,

$$x_1^*(t) = \exp(-(t-\tau))x_1^*(\tau), \tag{2.51a}$$

$$p_1^*(t) = 1 + \exp(t - \tau)(p_1^*(\tau) - 1). \tag{2.51b}$$

Substituting this in (2.38a) yields

$$\dot{\varphi}^*(t) = \exp(t - \tau)(p_1^*(\tau) - 1) + \exp(-(t - \tau))x_1^*(\tau)$$
(2.52a)

$$< \exp(t - \tau) \left( p_1^*(\tau) - 1 + x_1^*(\tau) \right),$$
 (2.52b)

where the last equation follows from the fact that along the periodic solution  $x_1^*(s) \in (0,1)$  for all s. Combining this with (2.50) implies that

$$\dot{\varphi}^*(t) < 0 \text{ for all } t \in (\tau, \tau + \varepsilon).$$
 (2.53)

This clearly implies that  $\varphi^*(t) < 0$  for all  $t \in (\tau, T]$ . Thus, the concatenations  $B_+B_-S$  and  $B_+B_-B_+$  are not possible. A similar argument shows that if  $u^*$  includes  $B_-B_+$  then the concatenations  $B_-B_+S$  and  $B_-B_+B_-$  are not possible.

The analysis above implies that the most general form possible for an optimal control is

$$B_1SB_2B_3,$$
 (2.54)

where every  $B_i$  stands for wither  $B_-$  or  $B_+$ . Our next goal is to compare a control u with such a structure to the control that includes a single singular arc. To do this, it is necessary to explicitly compute and compare the cost J along such controls. The following lemma is used in the solution of a scalar switched system.

**Lemma 6.** Pick  $b_1 > b_2 > 0$  and  $a_1, a_2 \in \mathbb{R}$ . Suppose that starting from  $y(0) = y_0$  and follow the dynamics  $\dot{y} = a_1 - b_1 y$  for  $t \in [0, t_1]$ , with  $t_1 > 0$ , and then switch to  $\dot{y} = a_2 - b_2 y$  for  $t \in [t_1, t_1 + t_2]$ , with  $t_2 > 0$ , and such that  $y(t_1 + t_2) = y_0$  (that is, the system returns to its initial state). Then

$$\int_{0}^{t_1+t_2} y(t) dt < t_1 c_1 + t_2 c_2 + \frac{t_1 t_2 (b_1 - b_2)(c_1 - c_2)}{b_1 t_1 + b_2 t_2}, \tag{2.55}$$

where  $c_i := a_i/b_i$ .

*Proof.* First consider the scalar equation  $\dot{y} = a - by$ , with  $b \neq 0$ ,  $y(t_0) = y_0$  and  $y(t_1) = y_1$ . Then integration yields

$$y_1 - y_0 = \int_{t_0}^{t_1} (a - by(t)) dt = a(t_1 - t_0) - b \int_{t_0}^{t_1} y(t) dt,$$
 (2.56)

SO

$$\int_{t_0}^{t_1} y(t) dt = (t_1 - t_0) \frac{a}{b} - \frac{y_1 - y_0}{b}.$$
 (2.57)

Now fix  $b_1 > b_2 > 0$ . Suppose that starting from  $y(0) = y_0$  we follow the dynamics  $\dot{y} = a_1 - b_1 y$  for  $t \in [0, t_1]$ , with  $t_1 > 0$ , and then switch to  $\dot{y} = a_2 - b_2 y$  for  $t \in [t_1, t_1 + t_2]$ , with  $t_2 > 0$ , such that  $y(t_1 + t_2) = y_0$ . That is, the system returns to its initial state. Then

$$y(t_1) = c_1(1 - \exp(-b_1t_1)) + \exp(-b_1t_1)y_0, \tag{2.58a}$$

$$y(t_1 + t_2) = c_2(1 - \exp(-b_2 t_2)) + \exp(-b_2 t_2)y(t_1), \tag{2.58b}$$

where  $c_i := a_i/b_i$ . Denoting  $y_1 := y(t_1)$  and using the fact that  $y(t_1 + t_2) = y_0$  yields

$$y_1 = c_1(1 - \exp(-b_1t_1)) + \exp(-b_1t_1)(c_2(1 - \exp(-b_2t_2))) + \exp(-b_2t_2)y_1),$$
 (2.59a)

$$y_0 = c_2(1 - \exp(-b_2t_2)) + \exp(-b_2t_2) (c_1(1 - \exp(-b_1t_1)) + \exp(-b_1t_1)y_0),$$
 (2.59b)

so

$$y_1 - y_0 = (c_1 - c_2) \frac{(1 - \exp(-b_1 t_1))(1 - \exp(-b_2 t_2))}{1 - \exp(-b_1 t_1 - b_2 t_2)}.$$
 (2.60)

It is straightforward to show that for any v, w > 0 we have

$$\frac{(1 - \exp(-v))(1 - \exp(-w))}{1 - \exp(-(v + w))} < \frac{vw}{v + w},\tag{2.61}$$

so we obtain the bound

$$y_1 - y_0 < (c_1 - c_2) \frac{b_1 b_2 t_1 t_2}{b_1 t_1 + b_2 t_2}. (2.62)$$

On the other-hand, (2.57) yields

$$\int_0^{t_1+t_2} y(t) \, \mathrm{d}t = \int_0^{t_1} y(t) \, \mathrm{d}t + \int_{t_1}^{t_1+t_2} y(t) \, \mathrm{d}t$$
 (2.63a)

$$=t_1c_1 - \frac{y_1 - y_0}{b_1} + t_2c_2 - \frac{y_0 - y_1}{b_2}$$
 (2.63b)

$$= t_1c_1 + t_2c_2 + (y_1 - y_0)(b_2^{-1} - b_1^{-1}). (2.63c)$$

Using (2.62) and the fact that  $b_1 > b_2 > 0$  yields (2.55) and this completes the proof.  $\Box$ 

The next result completes the proof of Theorem 1.

**Lemma 7.** If  $u^*$  has the form (2.54) then  $u^*$  includes a single singular arc.

#### 2.4 A single stage RFM with two inputs

Consider the scalar system with two inputs over a compact time interval [0, T]:

$$\dot{x} = u_0(t)(1 - x(t)) - u_1(t)x(t),$$

with the integral constraints  $\int_0^T u_0(t)dt = T\bar{u}_0$ ,  $\int_0^T u_1(t)dt = T\bar{u}_1$ . The one-dimensional problem with integral constraints can be lifted to a three dimensional system with boundary conditions as follows:

$$\dot{x}_1(t) = u_0(t)(1 - x_1(t)) - u_1 x_1(t), \tag{2.64a}$$

$$\dot{x}_2(t) = u_0(t), \tag{2.64b}$$

$$\dot{x}_3(t) = u_1(t). {(2.64c)}$$

with the boundary conditions

$$x_1(T) = x_1(0), \ x_2(0) = 0, \ x_2(T) = T\bar{u}_0, \ x_3(0) = 0, \ x_3(T) = T\bar{u}_1.$$
 (2.65)

Given two positive numbers  $\ell, L$  with  $\ell < L$ , the optimal control problem can be stated as follows:

**Problem 3.** Find  $u_0, u_1 : [0, T] \to [\ell, L]$  that maximizes the cost functional

$$J := \frac{1}{T} \int_0^T u_1(t) x_1(t) dt, \tag{2.66}$$

subject to the dynamics (2.64a) and the boundary conditions (2.65).

The result can be stated as follows:

**Theorem 8.** For any  $\ell$ , L with  $0 < \ell \le \bar{u}_0/(\bar{u}_1 + \bar{u}_0) \le L$ , the optimal cost for Problem 3 is

$$J^* = \frac{\bar{u}_0}{\bar{u}_1 + \bar{u}_0}. (2.67)$$

and it can be achieved by the following inputs:

$$u_0^*(t) \equiv \bar{u}_0, u_1^*(t) \equiv \bar{u}_1.$$
 (2.68)

**Remark 1.** The control inputs that achieve the optimal cost are not unique, since if the two control inputs are coupled via the equation  $u_0(t)/\bar{u}_0 \equiv u_1(t)/\bar{u}_1$  then system will be given by:

$$\dot{x}_1(t) = u_0(t) \left( 1 - \frac{\bar{u}_1 + \bar{u}_0}{\bar{u}_0} x_1(t) \right).$$

Then any measurable function  $u_0$  will achieve  $J^*$  given in (2.67).

#### 2.4.1 Pontryagin's maximum principle

Consider Problem 8, let the  $p(t) = [p_1(t), p_2(t), p_3(t)]$  be the accompanying co-state vector. The associated Hamiltonian can be written as:

$$\mathcal{H} = (p_1(t)(1 - x_1(t)) + p_2(t))u_0(t) + (x_1(t)(1 - p_1(t)) + p_3(t))u_1(t). \tag{2.69}$$

The time-evolution of the co-state is given by the following ODE:

$$\dot{p} = \begin{bmatrix} (u_0(t) + u_1(t))p_1(t) - u_1(t) \\ 0 \\ 0 \end{bmatrix}, \tag{2.70}$$

with the boundary condition  $p_1(0) = p_1(1)$ .

Hence, two of the co-states are constants and are given by

$$p_2(t) \equiv p_2(0), p_3(t) \equiv p_3(0).$$
 (2.71)

In what follows, let  $\mathscr{X}:=(u_0^*(t),u_1^*(t),x^*(t),p^*(t))$  be an optimal trajectory. We first state the following lemma:

**Lemma 9.** Let  $\mathscr X$  be an optimal trajectory. Then  $x_1^*(t), p_1^*(t) \in (\frac{\ell}{L+\ell}, \frac{L}{\ell+L})$  for all  $t \in [0, T]$ .

Proof. For the sake of contradiction, assume that  $x(0) > L/(L+\ell)$ . Since  $u_0, u_1 \in [\ell, L]$ , the comparison principle implies  $\dot{x}(t) > 0$  for all t. Hence x(T) > x(t), which contradicts x(T) = x(0). The argument can be repeated if  $x(0) < \ell/(L+\ell)$ . Hence  $x(0) = x(T) \in (\frac{\ell}{L+\ell}, \frac{L}{\ell+L})$ . Now assume that  $\exists t^* \in (0,T)$  such that  $x(t^*) > L/L + \ell > x(T)$ , the same argument shows that x(t) > x(T) for all  $t \in (t^*,T]$  which is a contradiction. The argument can be repeated if  $x(t^*) < \ell/(L+\ell)$ . A similar argument can be made to prove the corresponding statement for  $p_1(t)$ .

#### 2.4.2 Characterization of of regular arcs

Rhere are two inputs, so there are two switching functions:

$$\varphi_0(t) = p_1(1 - x_1) + p_2(0) \tag{2.72a}$$

$$\varphi_1(t) = x_1(1 - p_1) + p_3(0).$$
 (2.72b)

A regular arc is one in which the switching functions do not vanish when evaluated at it. Since the Hamiltonian is linear in the control input, then the optimal control is bang-bang when the switching function does not vanish. This is stated in the following the Lemma:

**Lemma 10.** Let  $\mathscr{X}$  be an optimal trajectory, then if  $\varphi_i(t) \neq 0$ , i = 0, 1 then:

$$u_i^*(t) = \begin{cases} L : \varphi_i(t) > 0 \\ \ell : \varphi_i(t) < 0 \end{cases}, \tag{2.73}$$

i.e,  $u_i(t)$  is a bang-bang control when corresponding switching function does not vanish.

*Proof.* Without loss of generality, let i = 0. Let  $\varphi_0(t) > 0$ , and let  $u_0^*(t) < L$ . However,

$$\mathcal{H}(u_0^*(t), u_1^*(t), x^*(t), p^*(t)) = \varphi_1(t)u_1^*(t) + \varphi_0(t)u_0^*(t) < \varphi_1(t)u_1^*(t) + \varphi_0(t)L = \mathcal{H}(L, u_1^*(t), x^*(t), p^*(t)),$$
(2.74)

which violates condition 3 in Proposition 2. Hence,  $u_0^*(t) < L$  is not optimal. The same argument can be applied when  $\varphi_0(t) < 0$ , and also for i = 1.

#### 2.4.3 Characterization of of singular arcs

Given an optimal trajectory  $\mathcal{X}$ , let

$$E^{i}_{+} := \{ t \in [0, T] : \varphi_{i}^{*}(t) > 0 \}, \tag{2.75a}$$

$$E_{-}^{i} := \{ t \in [0, T] : \varphi_{i}^{*}(t) < 0 \}, \tag{2.75b}$$

$$E_0^i := \{ t \in [0, T] : \varphi_i^*(t) = 0 \}, \tag{2.75c}$$

where i = 0, 1. Note that all these sets are measurable.

We also need the time derivatives of the switching functions:

$$\dot{\varphi}_0(t) = u_1(t)(p_1 - (1 - x_1)) \tag{2.76a}$$

$$\dot{\varphi}_1(t) = u_0(t)(1 - x_1 - p_1). \tag{2.76b}$$

Note that  $\dot{\varphi}_0$ ,  $\dot{\varphi}_1$  are bounded, and continuous almost everywhere. Note also that the  $sgn(\dot{\varphi}_0(t)) = -sgn(\dot{\varphi}_1(t))$ , which will be used later.

In this subsection the interest is in the case with  $\mu(E_0^i) > 0$  for either i = 0 or i = 1. A few lemmas are provided to characterize the system behaviour in such case.

**Lemma 11.** Let  $\mathscr X$  be an optimal trajectory, and assume that  $\mu(E_0^i) > 0$  for  $i \in \{0,1\}$ . Then there exists  $c_i \in (\frac{\ell}{L+\ell}, \frac{L}{\ell+L})$  such that

$$x_1^*(t) \equiv c_i \text{ for all } t \in E_0^{i'}. \tag{2.77}$$

where  $E_0^{i'}$  is the set of accumulation points of  $E_0^i$ . Furthermore, the two inputs must be satisfying the following relationship:

$$u_0(t) \equiv \frac{c_i}{1 - c_i} u_1(t), t \in E_0^{i'}. \tag{2.78}$$

Proof. Let  $E_0^{i'}\subseteq E_0^i$  denote the set of accumulation points of  $E_0^i$ . Note that  $\mu(E_0^{i,'})=\mu(E_0^i)$ , since  $E_0^i-E_0^{i'}$  is the set of isolated points of  $E_0^i$  which is countable, and hence has measure zero. For  $t\in E_0^{i'}$ , the  $\varphi_i^*(t)=0$ , so  $(\varphi^*(t))^{(k)}:=\frac{d^k}{dt^k}\varphi^*(t)=0$  for any integer  $k\geq 0$ .

W.l.o.g, let i=0, The equation  $\varphi_0^*(t)=\dot{\varphi}_0^*(t)=0$  yields  $p_1^*(t)(1-x_1^*(t))\equiv -p_2^*(0)$ , and  $p_1^*(t)\equiv 1-x_1^*(t)$ . In conclusion

$$p_1^*(t) \equiv 1 - x_1^*(t) \equiv 1 - c_0, \tag{2.79}$$

where  $c_0$  is a constant. Since  $x^*(t) \in (0,1)$ ,  $r \in (0,1)$ . Hence,  $p_2^*(0) = -c_0^2 < 0$ . The same argument can be repeated when i = 1.

Since 
$$x_1(t)$$
 is constant, then  $\dot{x}(t) \equiv 0$  and (2.78) follows.

The results above leave the possibility that  $c_0 \neq c_1$ . The following lemma provides further restrictions.

**Lemma 12.** Let  $\mathcal{X}$  be an optimal trajectory. Then:

1. If 
$$\mu(E_0^0 \cap E_0^1) > 0$$
, then  $E_0^{0'} = E_0^{1'}$ , and  $\exists c \in (0,1)$  such that  $x(t) \equiv c$  when  $t \in E_0^{0'}$ .

2. If  $\mu(E_0^0 \cap E_0^1) = 0$ , and  $\mu(E_0^0) > 0$ . Then  $\dot{\varphi}_1(t) \equiv 0$  and there exists a constant  $\bar{\varphi}_1 \neq 0$  such that  $\varphi_1(t) = \bar{\varphi}_1 \neq 0$  on  $t \in E_0^{0'}$ . A parallel statement hold be exchanging i = 0 with i = 1.

*Proof.* The two statements can be proved as follows:

- 1. Let  $c_0, c_1$  be given as in Lemma 11. Since  $\mu(E_0^0 \cap E_0^1) > 0$ , then  $c_0 = c_1$ , which also uniquely determines  $p_2(0), p_3(0)$ . Hence,  $E_0^{0'} = E_0^{1'}$ .
- 2. The assumptions imply that  $\varphi_0^*(t) = \dot{\varphi}_0^*(t) \equiv 0$  for  $t \in E_0^{0'}$ . Using (2.76a),(2.76b), it can be written that  $\dot{\varphi}_1(t)=0$  if  $\dot{\varphi}_0(t)=0$ . Since  $x(t),p_1(t)$  on  $E_0^{0'}$  are constant hence  $\varphi_1(t) \equiv \bar{\varphi}_1 := c_0^2 + \lambda_3(0).$

The last lemma shows that an optimal trajectory has two disjoint case for the singular arcs. Either each singular arc has both switching functions vanishing together, or only one of them can vanish at a time.

#### **Admissible Switching Patterns** 2.4.4

In the previous subsection we have shown that the optimal control can either be a bangbang or singular. On the singular arc, the controls need to satisfy (2.78) but the state is constant, hence the value of the free input has no effect on the dynamics since  $\dot{x}_1 = 0$  on all singular arcs. In general, there can be an arbitrary switching between these cases. In this part, the class of admissible switching patterns become more restricted.

Assuming that control inputs are *piecewise continuous*, and hence the switching functions are piecewise differentiable. An arc is the restriction of the optimal trajectory  $\mathscr{X}$  onto a maximal time interval such that the switching functions have a constant sign on that interval. Hence, the optimal trajectory  $\mathscr{X}$  can be decomposed into a sequences of arcs.

In order to facilitate the discussion we define the concept of an arc sign as an ordered pair. An arc has a sign  $s=(s_0,s_1)\in \mathscr{S}^2:=\{0,+,-\}^2 \text{ iff } \operatorname{sgn}(\varphi_i(t))\equiv s_i \text{ for } i=0,1.$  Let  $s^j, s^k$  be the signs of two consecutive arcs. An arc transition is an ordered tuple of arc signs, and is represented as follows:  $s^j \to s^k$ . The reverse of an arc transition  $s^j \to s^k$  is  $s^k \to s^j$ . A switching transition is said to be *inadmissible* if it can not occur in an optimal trajectory.

Some arc transitions are excluded in the following lemma:

**Lemma 13.** Let  $\mathscr{X}$  be an optimal trajectory. Then the following arc transitions and their reverses are inadmissible:  $(+,+) \to (-,-)$ ,  $(0,0) \to (+,+)$ ,  $(0,0) \to (-,-)$ .

*Proof.* Consider two consecutive arcs with a transition time  $\tau$ . Hence, there exists  $\varepsilon>0$  such that the first arc defined on a time interval  $(\tau-\varepsilon,\tau)$  with sign (+,+), and second arc defined on  $(\tau,\tau+\varepsilon)$  with sign (-,-). Since both switching functions change sign from positive to negative at  $\tau$ , then we have  $D_{\tau}^{+}\varphi_{i}(t)\leq0$ , i=0,1, where  $D_{\tau}^{+}$  is the upper right Dini's derivative at  $\tau^{-1}$ . This also implies that  $\exists \varepsilon_{2}\leq\varepsilon$  such that  $\dot{\varphi}_{i}(t)<0$  for  $t\in(\tau,\tau+\varepsilon_{2}), i=0,1$ . But this contradicts (2.76a),(2.76b) which imply that  $\mathrm{sgn}(\dot{\varphi}_{0}(t))=-\mathrm{sgn}(\dot{\varphi}_{1}(t))$ . So this means that transition  $(+,+)\to(-,-)$  can not be realized by any trajectory, including an optimal trajectory  $\mathscr{X}$ .

A similar argument can be provided for all other cases.

Let  $(s_0, s_1)$  be the sign of an arc. An arc sign's entry  $s_i$  is said to be *locked* to  $s \in \mathscr{S}$  if all subsequent arcs have signs with  $s_i = s$ . An arc sign's entry written as  $\Box s$  means that entry is locked to  $s \in \mathscr{S}$ . For example, an arc with the sign  $(\Box +, -)$  means that all subsequent arcs have a sign of the form (+, s) for some  $s \in \mathscr{S}$ . The notation  $(s_0, s_1) \to (\Box s, s^*)$  means that the transition result in the first entry being locked to s. Similarly  $(s_0, s_1) \to (s^*, \Box s)$  means that the second entry will be locked to s.

The following lemma is based on the notation introduced above:

**Lemma 14.** Let  $\mathscr{X}$  be an optimal trajectory, and consider two consecutive arcs. Then  $\forall s \in \mathscr{S}$ , a transition of the form  $(+,s) \to (-,+)$  is equivalent to  $(+,s) \to (\boxminus,+)$ . The parallel statements also hold with  $(-,s) \to (\boxminus,-), (s,+) \to (+,\boxminus), (s,-) \to (-,\boxminus)$ .

*Proof.* Consider the transition  $(+,s) \to (-,+)$ , and let  $\tau$  be the transition time. Then,  $\varphi_0(t) > 0$  on  $(\tau - \varepsilon_2, \tau)$  and  $\varphi_0(t) < 0$  on  $(\tau, \tau + \varepsilon_1)$ , where  $\varepsilon_1, \varepsilon_2 > 0$  are the duration of each of the two arcs, respectively. By Lemma 10, we have  $u_0(t) \equiv \ell, u_1(t) \equiv L$  for  $t \in (\tau, \tau + \varepsilon_1)$ . Similar to the proof of the previous lemma,  $D_{\tau}^+ \varphi_0(t) \leq 0$ , which can be written as follows:

$$D_{\tau}^{+}\varphi_{0}(t) = u_{1}(\tau_{+})(p_{1}(\tau) - (1 - x_{1}(\tau))) = L(p_{1}(\tau) - (1 - x_{1}(\tau))) \le 0,$$

$$(2.80)$$

$$D_{\tau}^{+}\varphi(t) := \limsup_{t \to 0^{+}} (\varphi(\tau + h) - \varphi(\tau))/h.$$

Recall that  $\dot{x}_1 = u_0 - (u_0 + u_1)x_1, \dot{p} = (u_0 + u_1)p - u_1$ . Following on  $t \in (\tau, \tau + \varepsilon_1)$ :

$$x(t) = \left(x(\tau) - \frac{\ell}{\ell + L}\right)e^{-(\ell + L)(t - \tau)} + \frac{\ell}{\ell + L} < \left(x(\tau) - \frac{\ell}{\ell + L}\right)e^{(\ell + L)(t - \tau)} + \frac{\ell}{\ell + L}$$
(2.81a)

$$p(t) = \left(p(\tau) - \frac{L}{\ell + L}\right) e^{(\ell + L)(t - \tau)} + \frac{L}{\ell + L},\tag{2.81b}$$

where the inequality (2.81a) follows since  $x(t) > \frac{\ell}{\ell + L}$  by Lemma 9.

Consdiering the derivative of the switching function on  $(\tau, \tau + \varepsilon_1)$  and use inequalities (2.81a), (2.80) as follows:

$$\dot{\varphi}_0(t) = L(p_1(t) + x_1(t) - 1) < L(x(\tau) + p(\tau) - 1)e^{(\ell + L)(t - \tau)} \le 0.$$
(2.82)

Hence,  $\dot{\varphi}_0(t) < 0$  on  $(\tau, \tau + \varepsilon_1)$ . From  $\varphi_0(\tau) = 0$ , and integrating

$$\varphi_0(t) < 0 \text{ for } t \in (\tau, \tau + \varepsilon_1).$$
 (2.83)

The claim is that this implies that  $u_0(t) = \ell$  for  $t \in (\tau, T]$ . The proof is: For the sake of contradiction assume that  $u_0(\tau + \varepsilon_1) = L$ . By Lemma 10, this is only optimal if  $\varphi_0(\tau + \varepsilon_1) > 0$  which contradicts (2.83) since  $\varphi_0$  is continuous. Hence  $(+, s_1) \to (-, +) \to (+, s_2)$  is not admissible for any  $s_1, s_2 \in \mathscr{S}$ . Similarly,  $(+, s_1) \to (-, +) \to (0, s_2)$  is not possible since it violates continuity of  $\varphi_0$ . Hence  $(+, s) \to (-, +)$  is equivalent to  $(+, s) \to (\square, +)$ .

Similar arguments can be repeated for the other cases.

There are other transitions should be excluded. They are stated in the following two lemmas:

**Lemma 15.** Let  $\mathscr{X}$  be an optimal trajectory. Consider two consecutive arcs. The following transition is not admissible:  $(+,0) \to (-,s)$ , for any  $s \in \mathscr{S}$ . Similarly,  $(+,0) \to (0,s)$ ,  $(-,0) \to (+,s)$ ,  $(-,0) \to (0,s)$ ,  $(0,+) \to (s,-)$ ,  $(0,+) \to (s,0)$ ,  $(0,-) \to (s,+)$ ,  $(0,-) \to (s,0)$  for any  $s \in \mathscr{S}$ . Also, all their reverses.

*Proof.* W.l.o.g, let's have the transition  $(0,+) \to (+,0)$ . Let  $\tau$  be the transition time. There exists  $\varepsilon > 0$  such that  $\varphi_1(t) \equiv 0$  for  $t \in (t,t+\varepsilon)$ , and (by Lemma 12)  $\varphi_1(t) \equiv \bar{\varphi}_1 > 0$  for  $t \in (\tau-\varepsilon,\tau)$ . This implies that  $\varphi_1(t)$  is discontinuous at  $\tau$ ; a contradiction. The same argument can be used for the other cases.

**Lemma 16.** Let  $\mathscr{X}$  be an optimal trajectory, and consider three consecutive arcs. Then, the following transition is inadmissible:  $(+,0) \to (+,+) \to (+,0)$ . Similarly, the following transitions are inadmissible  $(0,+) \to (+,+) \to (0,+)$ ,  $(-,0) \to (-,-) \to (-,0)$ ,  $(0,-) \to (-,-) \to (0,-)$ 

*Proof.* Let the arcs be defined on the following time intervals  $(\tau_1 - \varepsilon_1, \tau_1), (\tau_1, \tau_2), (\tau_2, \tau_2 + \varepsilon_2)$  for some  $\tau_1, \tau_2, \varepsilon_1, \varepsilon_2 > 0$ . Then on the first arc, Lemma 11 gives that  $x_1(t) \equiv c_0$  for  $t \in (\tau_1 - \varepsilon_1, \tau_1)$ . On the second arc, the system is represented by  $\dot{x}_1 = L(1-2x)$ , with  $x(\tau_1) = c_0$ , and the third arc we have  $x(\tau_2) \equiv c_0$  for  $t \in (\tau_2, \tau_2 + \varepsilon)$ . If  $c_0 \neq \frac{1}{2}$ , then it follows  $x_1$  is discontinuous at  $\tau_2$ ; a contradiction. If  $c_0 = \frac{1}{2}$ , then this implies that  $x_1(t) \equiv c_0$  on the second arc which implies that  $\varphi_0(t) \equiv 0$  on that arc, i.e it has a sign (0, +); a contradiction. The proof is similar for the remaining cases.

Using Lemma 12, If an optimal trajectory has an arc with the sign (0,0), then it can not have arcs with signs  $(\pm,0)$  or  $(0,\pm)$ . Using the above lemmas, there is no cycle possible amongst the arc signs. So,

**Proposition 17.** Let  $\mathscr{X}$  be an optimal trajectory. Then, it can not have more than 9 arcs.

The proof consists of starting from an arc sign, and then tracing the longest possible arc transitions. All such paths will terminate, and the longest one can be found. For instance, if the optimal trajectory  $\mathscr X$  has an arc with sign (0,0), then the transition diagram is simple. If the trajectory starts from (+,-) then the longest paths are as follows:

$$(+,-) \rightarrow (0,0) - (\square,\square)$$

A similar diagram can be given if the trajectory starts from (-,+). If it starts from (+,+) or (-,-) then (0,0) cannot appear, and the diagram will be a subset of the diagram in the second case that follows.

The second case is when singular arcs can be present but without an arc with the sign (0,0). The longest path diagram is as follows:

$$(+,-) \rightarrow (+,+) \rightarrow (+,0) \rightarrow (+,+) - (\square,+) \rightarrow (\square,-) \rightarrow (\square,\square)$$

$$(+,-) \rightarrow (+,+) \rightarrow (+,0) \rightarrow (+,+) - (\square,+) \rightarrow (\square,-) \rightarrow (\square,-$$

All other transitions that share the first two arcs are subsets of these longer transitions above. For instance, if the trajectory starts from any of the first three arcs to get a diagram, or it can eliminate the singular arcs from the diagram above to get admissible trajectories consisting entirely of regular arcs. Also, the second arc's sign can be changed to (-, -) and a dual diagram can be given. Similar transition diagrams can be given when we start with (-, +) instead.

## 2.4.5 Suboptimality of admissible switching patterns

In this part, longest path, given in the previous sections, are shown to be suboptimal. The following tricks helps to reduce the number of cases that were provided in Prop. 17.

**Lemma 18.** Any trajectory with n arcs that is starting and ending with the same arc can be written with n-1 arcs without loss of generality.

*Proof.* Consider a trajectory that starts with  $(s_1, s_2)$  arc  $t \in (0, \tau_1)$  and finishes with  $(s_1, s_2)$  arc  $t \in (T - \tau_2, T)$ . By defining the period between for  $t \in (\tau_1, T + tau_1)$ . The trajectory starts with the 2nd arc at time  $\tau_1$  and finishes at time  $T + \tau_1$ , where the last arc's time length is  $\tau_1 + \tau_2$ .

The following lemma, helps to derive one integral for the four optimal trajectories that were defined in Prop. 17 and include an arc with sign (0,0).

**Lemma 19.** If the optimal trajectory  $\mathscr{X}$  has an arc with sign (0,0), then it can be written in the form of  $(+,-) \to (0,0) \to (-,+)$ .

*Proof.* From the Porp. 17 and Lemma 18, the optimal trajectory  $\mathscr{X}$  that has an arc with sign (0,0) can be written in the form of  $(0,0) \to (-,+)$ ,  $(0,0) \to (+,-)$ ,  $(+,-) \to (0,0) \to (-,+)$ , and  $(-,+) \to (0,0) \to (+,-)$ . The  $(0,0) \to (-,+)$ , and  $(-,+) \to (0,0) \to (+,-)$  trajectories contradict the periodicity of the optimal trajectory, while and  $(+,-) \to (0,0) \to (-,+)$  is equivalent to  $(-,+) \to (0,0) \to (+,-)$  by shifting the period to the starting time of the last arc of each trajectory.

Now, the cost function of Problem 3 can be driven, for the optimal trajectory that was defined in lemma 19. Consider that the (+,-) arc switches to (0,0) trajectory at  $\tau_1$ , then switches

to (-,+) at time  $T-\tau_2$ . The cost function would be:

$$J := \frac{1}{T} \int_{0}^{T} u_{1}(t)x_{1}(t)dt,$$

$$= \frac{1}{\tau_{1}} \int_{0}^{\tau_{1}} u_{1}(t)x_{1}(t)dt + \frac{1}{T - \tau_{1} - \tau_{2}} \int_{\tau_{1}}^{T - \tau_{2}} u_{1}(t)x_{1}(t)dt + \frac{1}{\tau_{2}} \int_{T - \tau_{2}}^{T} u_{1}(t)x_{1}(t)dt,$$
(2.84b)

$$= c_0 \mu(E^0) + c_+ \mu(E^+) + c_- \mu(E^-) + (c_+ - c_-)(b_+ - b_-) \sum_{i=1}^n \frac{t_i^+ t_i^-}{b_+ t_i^+ + b_- t_i^-}.$$
 (2.84c)

Considering the (10) values for - and + signs of the arc, and  $c_0$ ,  $c_1$  for the singular value sign 0. The boundary conditions (2.65) imply that:

$$\bar{u}_0 = \frac{L\tau_1 + c_0(T - \tau_1 - \tau_2) + l\tau_2}{T},$$
(2.85a)

$$\bar{u}_1 = \frac{l\tau_1 + c_1(T - \tau_1 - \tau_2) + L\tau_2}{T}.$$
 (2.85b)

## 2.5 Conclusion

If so, then may be we can call this the "casino effect" the gains are never enough to compensate for the losses. This means that entertainment to a (non-trivial) periodic signal always incurs a cost, as the production rate would have been better for constant signals.

An interesting research direction is to prove that for certain general classes of contractive systems the periodic gain is one. This may be done for example by considering cases where the PMP is not only a necessary condition for optimality, but also a sufficient condition.

An interesting goal is to derive a simple to test ad-hoc procedure for determining whether the periodic gain is larger or smaller than one. A simple idea in this direction is for the case of a single periodic rate, say  $\lambda(t)$ . Suppose that for a constant rate  $\lambda(t) \equiv a$  the steady-state output is f(a). Suppose also that  $f \in C^2$ , and that f'(a) > 0. For  $\varepsilon > 0$  sufficiently small, then

$$f(a+\varepsilon) - f(a) \approx \varepsilon f'(a) + \frac{\varepsilon^2}{2} f''(a) > 0,$$
 (2.86)

i.e. when increasing a to  $a + \varepsilon$  we increase the steady state-state by  $\varepsilon f'(a) + \frac{\varepsilon}{2} f''(a)$ . Similarly,

$$f(a-\varepsilon) - f(a) \approx -\varepsilon f'(a) + \frac{\varepsilon^2}{2} f''(a) < 0,$$
 (2.87)

i.e. when decreasing a to  $a-\varepsilon$ , to reduce the steady state-state by  $\varepsilon f'(a)-\frac{\varepsilon^2}{2}f''(a)$ . The "total gain" when a is varied in the range  $[a-\varepsilon,a+\varepsilon]$  is thus  $\varepsilon^2 f''(a)$ . The same result is obtained

when f'(a) < 0. This suggests that if f''(a) > 0 (f''(a) < 0) then the "total gain" is positive [negative] and it may be expected the periodic gain (for rates that vary around an average a) to be larger [smaller] than one.

To demonstrate this, note that for the RFM with n=1 and  $\lambda=1$ , the steady-state production rate  $R=f(\lambda_0)$  with

$$f(\lambda_0) := \frac{\lambda_0}{1 + \lambda_0},\tag{2.88}$$

so

$$f''(\lambda_0) = \frac{-2}{(1+\lambda_0)^3} < 0, (2.89)$$

and this agrees with the fact that the periodic gain is smaller than one.

On the other-hand, for the system in Example ??, for  $u(t) \equiv a$ , with a > 0, the output is f(a) := 1/a, so

$$f''(a) = 2a^{-3} > 0, (2.90)$$

and this agrees with the fact that the periodic gain is larger than one.

## **Chapter 3**

# **Bispecific T-cell engagers**

Bispecific T cell engagers have proven to be a potent antibody design in cancer immunooncology by forming a trinary complex when binding to an immune cell and a cancer cell simultaneously. This type of antibody substitutes the role of antigen presenting cells to activate the immune cells against the cancer cells. T cell engagers should be carefully designed to have maximum potency, the immune cell-antibody-cancer cell trinary complex concentration, against tumor cells and circumvent cytokine storm in the body. A relatively high concentration of the antibody, increases the risk of cytokine storm, saturates the number of immune cell-antibody and antibody-cancer cell dimers, and hinders a potent response. A low concentration of the antibody is not sufficient to produce a potent concentration of trinary complex to activate the immune system against the cancer cells. The purpose of this study is to quantitatively investigate how the concentration of trinary complex, and distribution are dependent on the design characteristics of the bispecific antibodies, like the binding kinetics to the target receptors on the immune cells and the cancer cells. Several antibodies that are either clinically approved, or currently under clinical/preclinical development process are simulated to explore if the kinetics can be enhanced with a different design. Moreover, the identifiability analysis done in this work proves the sufficiency of steady state data for identifiability of the dissociation rates.

## 3.1 Introduction

BiTE has shown an strong cancer immunotherapy strategy in recent years [40–43]. BiTE technology has been proposed for treating acute myeloid leukemia [44], multiple myeloma [45], lymphoblastic leukemia [46], refractory solid tumors [47], and as a platform for targeted therapy

across different tumor types [48]. A list of BiTE molecules that were considered in this study is presented in table 3.1. This list is made by selecting the BiTE molecules that their binding kinetics to the targets were specified in the literature. More detailed review of the existing BiTEs or bispecific antibodies has been recently done recently by [43, 49, 50].

The targeted receptor protein of cancer cells are biomarkers of the cancer cells that have minimal expression in normal cells to have minimum off target effects. Also, BiTEs might have different chemical structure formats with different number of binding sites. The targeted receptor protein of immune cell is CD3 receptor of T cells for all the BiTEs considered in this study.

A three-body model [51] is what all bispecific antibodies have in common. In the three-body model a bispecific antibody, binding species, connects to two different target molecules, terminal species, to form a trinary complex. After the formation of dimers of the first target and the anibody, the binding kinetics can be changed based on Cooperativity factor to increase/decrease the binding affinity of the antibody molecule of the formed dimer to the second target. A positive Cooperativity factor increases the binding affinity, and it can be interpreted as the avidity factor explained in the bispecific antibody literature [52–55], where the bispecific antibody is targeting two different receptors of the same cell type for an increased specificity. The Cooperativity factor can be neglected in models of bispecific antibodies that are targeting two different cell types like BiTE, as the dimers are free in the spatial coordinates to bind to the second target. In this study, the first objective is to evaluate the design characteristics of BiTEs based on the simple model presented in figure 3.1. The BiTE antibody, X, is targeting receptors on the immune cells,  $T_1$  which usually is the CD3 receptor of T cells, and the protein receptor of cancer cells,  $T_2$ .

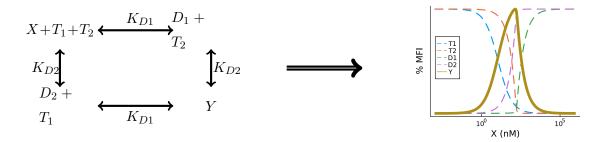


Figure 3.1: On the left side, the three-body model of BiTE, X,  $T_1$  and  $T_2$  are the two target receptors on immune and cancer cells,  $D_1$  and  $D_2$  are the dimers of bispecific antibody-immune cell and bispecific antibody-cancer cell, Y is the trimer complex, and  $k_{D1}$  and  $k_{D2}$  are the dissociation constants of the antibody binding equilibrium. The chemical reactions are visualized in a simple form to provide an intuitive idea of the reactions, specifically  $T_2$  ( $T_1$ ) is not involved in dimerization reaction between X and  $T_1(T_2)$ , i.e. the differential equations presented in (3.1) do not follow mass-action kinetics from the visualized chemical reaction network. On the right side, a nominal bell-shape pattern of the trinary complex Y in fluorescent intensity is visualized as a function of BiTE concentration. Binding kinetics and initial conditions are adopted from [56].

Table 3.1: CD3 BiTEs (sorted by the year of the referenced publication)

CD3 BiTE	Target	$k_{D1}(\mathrm{nM})$	$k_{D2}(\mathrm{nM})$	Type	Format	kDa	Ref
Blinatumomab	CD19	$\sim 100$		Liquid	BiTE	54	[57]
Solitomab	Ep-CAM	$16 \pm 12$		Liquid	BiTE	55	[58]
BAY2010112	PSMA	$9.4 \pm 4.3$		Solid	BiTE	55	[65]
PF-06671008	Pcad	$11.5\pm0.9$	$\overline{}$	Solid	DART	57	[09]
${ m CD3}_{arepsilon}{ m L/HER2}$	HER2	20		Solid	KIH	> 100	[61]
${ m CD3}_{arepsilon}{ m H/HER2}$	HER2	0.5		Solid	KIH	> 100	[61]
${ m CD3}_{arepsilon}{ m VH/HER2}$	HER2	0.05		Solid	KIH	> 100	[61]
7370	FLT3	27		Liquid	IgG-based	146	[62]
PF-07062119	<b>GUCY2C</b>	$7.47 \pm 0.15$	$23.97 \pm 0.97$	Solid	IgG1-FcyR	> 100	[63]
Tarlatamab	DLL3	$0.64 \pm 0.05$		Solid	HLE-BiTE	> 100	[64]
Acapatamab	PSMA	$22.4\pm2.8$		Solid	HLE-BiTE	> 100	[65]
Anti-CD79b/CD3	CD79b	12.8		Liquid	KIH	150	[99]

In the recent investigations such as [51, 56] it has been emphasised that the efficacy of BiTE, trimer concentration at the cite of action, is a bell-shape function. A relatively low or high concentration of a BiTE is not effective to produce enough number of trimer complexes to activate the immune cells against the cancer cells. At a low concentration the BiTE concentration is simply not enough to produce a potent concentration of trimer complex Y. At a high concentration the BiTE saturates the target receptor proteins on the immune cells and cancer cells, in a way that the dimers of immune cell - BiTE,  $D_1$ , and BiTE - cancer cell,  $D_2$ , increase and limit the number of free targets to form the trinary complex Y. Besides that, a high concentration of the BiTE can potentially cause off target side effects in the body or end up in a cytokine storm of the immune system.

In order to reproduce the bell-shape pattern of the efficacy of the BiTE to their initial concentration, four critical parameters are necessary: 1) initial concentration of target 1  $T_1$ , 2) initial concentration of  $T_2$ , 3) binding kinetics/dissociation constant of the BiTE to target 1  $K_{D1}$ , and 4) dissociation constant  $K_{D2}$ . The initial concentration of  $T_1$  is dependent on the number of T cells in the body. Most of the BiTEs are targeting CD3 as  $T_1$  (see table 3.1), therefore the variability of this target is based on patient to patient immune system variability. The initial concentration of  $T_2$  is dependent on the tumor. As reported by the references presented in table 3.1, the initial concentration of tumor specific targets are generally considered to be less than  $5 \times 10^3$ /cell, and might be significantly different because of the fundamental difference across different cancer types. The main discussion of this study is based on the binding kinetics of the bispecific molecules.

The binding affinity of the BiTE to  $T_1$  (CD3 on the T cells) can be significantly smaller, comparable, or significantly larger than the binding affinity to  $T_2$  (targeted receptor protein on the cancer cells). For example, the binding affinity of Blinatumomab [57], PF-06671008 [60], and (7370) [62] to target receptor on the immune cells is great than its binding affinity to target receptor on the cancer cells. The binding affinities of Acapatamab [65], Solitomab [58], and PF-07062119 [63] to its targets is in a comparable range. On the other hand, BiTEs like BAY2010112 [59], Taralatamab [64], and REGN5458 [67] present a larger affinity to the cancer cell targets in comparison to the immune cell targets.

The binding kinetics of the BiTE molecules to each of the targets may also effect the distribution of this type of antibody at different tissues. The bio-distribution of CD3/HER2 T-cell-Dependent Bispecific (TDB), or BiTE, has been measured for different range of affinities to CD3 for the solid tumors in mouse models [61]. Recent discoveries suggest higher affinities to CD3 (lower dissociation rate  $k_{D1}$ ) increases the uptake in T cell tissues, e.g. Lymph nodes, and decreases the uptake at the cite of action, e.g. Tumor Micro-Environment (TME). Therefore, lower affinities of

BiTE antibody molecules to CD3 is favorable in treatments designed for solid tumors.

In addition to the BiTE molecules represented in Table 3.1, other molecules are presented in literature in details. PF-06863135 [68] (150 kDa), and AMG420 [45] (54 kDa) are both designed to target BCMA for patients diagnosed with multiple myeloma. Both of the molecules have similar dissociation rate to CD3, but different dissociation rate to BCMA, 0.1 and 0.04 nM respectively. The role of binding kinetics to BCMA is discussed as an important factor in the distribution of the molecule toward different tissues in [45]. Also, the authors of [69] discussed the design and bio-distribution of AMG211 (55 kDa), a CD3/CEA BiTE molecule for patients with advanced gastrointestinal adenocarcinomas. AMG211 has a significantly high dissociation rate to CD3 310 nM in comparison with its dissociation rate toward CEA 5.5 nM. The bio-distributions of these molecules are compared computationally by [70] based on two pore pore theory. The number of BiTE molecules in this manuscript are kept limited for the simplicity of the study, and presented figures.

In the following sections a minimal mathematical model is presented with quantitative analysis of the BiTE molecules that were publicly available in the literature. Although each of the molecules presented are designed for a different target receptor of cancer cell, the targets are assumed to be equally expressed on the cancer cell surface to have a quantitative measure of their differences. At the end, a full quantitative systems pharmacology model of a nominal BiTE is given for a broader discussion on other parameters that might significantly change the optimal dosing regimen of BiTE molecules.

## 3.2 Three-body model and the importance of binding kinetics

Three-body model can be considered as a minimal model for the BiTE antibodies. The physiological model simulates the instant number of produced trinary complex and the occupancy of the targeted receptors immediately after exposing the culture of immune cells and cancer cells to the the BiTE antibody. The degradation of the targets and antibody is neglected in this section. This is a reasonable assumption where the dissociation equilibrium is estimated to happen much faster than the receptor shedding and antibody degradation processes.

The presented model in Figure 3.1 includes six state variables to model the concentration of the BiTE antibody X(t), the target receptor on the surface of the immune cells  $T_1(t)$ , the target receptor on the surface of the cancer cells  $T_2(t)$ , the dimer complex of immune cell-antibody  $D_1(t)$ , the dimer complex of antibody-immune cell  $D_2(t)$ , and the trinary complex of immune cell-antibody-

cancer cell Y(t). The initial concentration of the dimer and trimer complexes are assumed to be zero at the starting point  $D_1(0) = D_2(0) = Y(0) = 0$ . The initial concentration of BiTE antibody X(t=0) is the dose concentration that is being discussed in this section. The dynamic formulation of the three-body problem for BiTE antibodies can be written the following form.

$$\dot{X} = -k_{n1}T_1X - k_{n2}T_2X + k_{f1}D_1 + k_{f2}D_2, \tag{3.1a}$$

$$\dot{T}_1 = -k_{n1}T_1X + k_{f1}D_1 - k_{n1}T_1D_2 + k_{f1}Y, \tag{3.1b}$$

$$\dot{T}_2 = -k_{n2}T_2X + k_{f2}D_2 - k_{n2}T_2D_1 + k_{f2}Y,$$
(3.1c)

$$\dot{D}_1 = k_{n1}T_1X - k_{f1}D_1 - k_{n2}T_2D_1 + k_{f2}Y, \tag{3.1d}$$

$$\dot{D}_2 = k_{n2}T_2X - k_{f2}D_2 - k_{n1}T_1D_2 + k_{f1}Y, \tag{3.1e}$$

$$\dot{Y} = k_{n1}T_1D_2 + k_{n2}T_2D_1 - (k_{f1} + k_{f2})Y. \tag{3.1f}$$

Note, the time functionality of the state variables is dropped for writing simplicity, and the dot sign on the top of each state variable on the left side represents the time derivative. Model 3.1 contains only four parameters:  $k_{n1}$ ,  $k_{f1}$ ,  $k_{n2}$ , and  $k_{f2}$ . The parameters reported from the preclinical measurements, e.g. surface resonance experiment, are based on dissociation constants of the two binding sites:

$$k_{D1} = k_{f1}/k_{n1}, (3.2a)$$

$$k_{D2} = k_{f2}/k_{n2}. (3.2b)$$

Dissociation constant  $k_D$  is enough to estimate the final concentration of each species in a two body binding solution, and different values of  $(k_n, k_f)$  that result in the same dissociation constant result in a faster/slower reactions to reach to the equilibrium concentration.

The steady state simulation of Model (3.1) can be a used for preclinical experiments on a dish where the formed trimer concentration at a constant time, after exposure of the BiTE to the culture of cancer cells and immune cells, is measured. Figure 3.2 represents numerical simulations with the same parameters of the Maximum Fluorescence Intensity (MFI) molecule introduced in [56]. Figures 3.2a and 3.2b are the results of the same numerical simulation setup, and different range of input, initial concentration of the BiTE molecule in the medium. The vertical axis in Figures 3.2a and 3.2b is normalized MFI. The bell-shape of the trimer projection is the focus of this section which represent existence of an optimal concentration of BiTE at the cite of action, e.g. in the MFI, to produce the maximum concentration of the trimer complex. Note how different the experimental

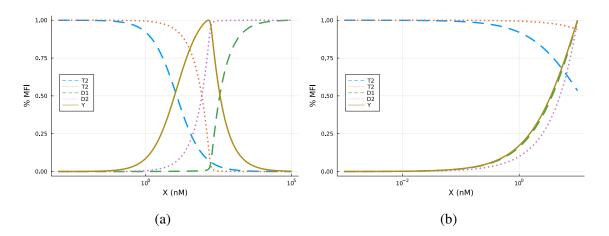


Figure 3.2: Steady state simulations of Model (3.1). The vertical axis is the normalized to the MFI levels of the variables in the experiments with different ranges of BiTE antibody initial concentration. The initial BiTE concentration range, range of horizontal axis values, in (a) is larger than (b). The plots on the left present the concentrations of the trimer and the targets, and the plots on the right side present the drug-target dimers concentrations.

results, e.g. Figure 3.2a vs Figure 3.2b, might look like when reported in MFI format with different range of MFI molecule concentration, drug dose on horizontal axis.

## 3.3 Identifiability

The structural identifiability analysis of model (3.1) based on a given drug X(t), the first target T1(t) (immune cells receptor), and the second target T2(t) (protein expressed on cancer cells) data is done. Results shows that all the parameters  $k_{n1}$ ,  $k_{f1}$ ,  $k_{n2}$ , and  $k_{f2}$  are globally and locally identifiable. The computer software SIAN [71], structural identifiability was used to confirm this result. On the contrary, most experimental measurements are done at the steady state [57–60, 62–65].

In the remainder of the identifiability analysis performed in this section, it is proved that the dissociation rates  $k_{D1} = k_{f1}/k_{n1}$ , and  $k_{D2} = k_{f2}/k_{n2}$  are identifiable for at most three steady state measurements. This result eliminates the need for extra measurements, e.g. surface resonance imaging, to determine the dissociation constants of BiTE molecules.

In terms of state variables Consider a steady state  $X^*$ ,  $T_1^*$ ,  $T_2^*$ ,  $D_1^*$ ,  $D_2^*$ ,  $Y^*$  of the system (3.1). Then the numbers  $X^*$ ,  $T_1^*$ ,  $T_2^*$ ,  $D_1^*$ ,  $D_2^*$ ,  $Y^*$ , and  $k_{n1}$ ,  $k_{n2}$ ,  $k_{f1}$ ,  $k_{f2}$  are related by a system of

six polynomial equations obtained by setting the left-hand sides of (3.1) to zero. To compute the projection of its solution set to  $(D_1^*, D_2^*, X^*, Y^*, k_{f1}, k_{f2})$ -coordinates (by performing elimination with Gröbner bases [72, Chapter 2, §1]) and find that the projection satisfies the following equation:

$$(D_1^*k_{f1} + D_2^*k_{f2} + X^*k_{f1} + X^*k_{f2})(D_1^*D_2^* - X^*Y^*) = 0.$$

Since the parameters and concentrations are positive, the left bracket does not vanish, so

$$X^* = \frac{D_1^* D_2^*}{V^*}. (3.3)$$

Adding this relation to the original system of six equations and computing the projections to the  $(D_1^*, D_2^*, Y^*, k_{f2}, k_{n2}, T_2^*)$ - and  $(D_1^*, D_2^*, Y^*, k_{f1}, k_{n1}, T_1^*)$ -coordinates, respectively, it can be obtained that

$$(D_1^*T_2^*k_{n_2} - Y^*k_{f_2})(D_1^* - D_2^*) = 0$$
, and  $(D_2^*T_1^*k_{n_1} - Y^*k_{f_1})(D_1^* - D_2^*) = 0$ .

For the generic case  $D_1^* \neq D_2^*$ ,

$$T_1^* = k_{D_1} \frac{Y^*}{D_2^*}, \quad \text{and} \quad T_2^* = k_{D_2} \frac{Y^*}{D_1^*}.$$
 (3.4)

In terms of first integrals The system (3.1) has three conservation laws, due to the constraints on the initial conditions:  $c_1 = T_1(t) + D_1(t) + Y(t)$ ,  $c_2 = T_2(t) + D_2(t) + Y(t)$ , and  $c_3 = X(t) + D_1(t) + D_2(t) + Y(t)$ . Based on the initial conditions,  $c_3 = X(0)$ . To prove that for every positive values of  $c_1, c_2, c_3$ , there exists at most one positive steady state, we augment the system obtained by setting the right-hand sides of (3.1) to zero with equations

$$c_1 - T_1^* - D_1^* - Y^* = c_2 - T_2^* - D_2^* - Y^* = c_3 - X^* - Y^* - D_1^* - D_2^* = 0.$$
 (3.5)

Given the obtained system of nine equations to compute the projections (again, using Gröbner bases) of the solution set to the  $(A, c_1, c_2, c_3, k_{D1}, k_{D2})$ -coordinates, where A is taken to be  $T_1^*$  or  $T_2^*$ , and find that these projections satisfy:

$$(T_1^*)^2 + (c_3 + k_{D1} - c_1)T_1^* - c_1k_{D1} = 0$$
 and  $(T_2^*)^2 + (c_3 + k_{D2} - c_2)T_2^* - c_2k_{D2} = 0$  (3.6)

Consider the first equation as a quadratic equation in  $T_1^*$ . The product of the roots is equal to  $-c_2k_{D2} < 0$ , so at most one of the roots is real positive, so  $T^*$  is uniquely determined. The same applies to  $T_1^*$ . Next, by computing projection to the  $(D_2^*, T_1^*, T_2^*, c_1, c_2, c_3, k_{D1}, k_{D2})$ -coordinates, to find the following relation for  $D_2^*$ :

$$c_3 D_2^* + T_1^* T_2^* - c_2 T_1^* - c_1 T_2^* + c_3 T_2^* + c_1 c_2 - c_2 c_3 = 0, (3.7)$$

which implies that  $D_2^*$  is uniquely determined. Finally,  $D_1^*, X^*$ , and  $Y^*$  are uniquely determined using the following simple consequences of (3.5):

$$D_1^* - D_2^* + T_1^* - T_2^* - c_1 + c_2 = 0$$
,  $Y^* + T_2^* + D_2^* - c_2 = 0$ , and  $X^* + D_2^* - T_1^* + c_1 - c_3 = 0$ . (3.8)

**Two experiments** Assuming that three experiments were conducted as described above and the steady state data  $(T_1^{[i]}, T_2^{[i]}, D^{[i]})$  is given for i = 1, 2, 3. The identification approach is to consider the first two experiments. Equations (3.3), and (3.4) are used to write the following polynomial system:

$$Y^{[i]}X^{[i]} = (c_1 - T_1^{[i]} - Y^{[i]})(c_2 - T_2^{[i]} - Y^{[i]}),$$
(3.9a)

$$T_1^{[i]}X^{[i]} = k_{D1}(c_1 - T_1^{[i]} - Y^{[i]}), (3.9b)$$

$$T_2^{[i]}X^{[i]} = k_{D2}(c_2 - T_2^{[i]} - Y^{[i]}),$$
 (3.9c)

for 
$$i = 1, 2$$
. (3.9d)

To compute the projection of the solution set of this system to the  $(k_{D1}, k_{D2}, T_1^{[1]}, T_1^{[2]}, T_2^{[1]}, T_2^{[2]}, X_2^{[1]}, X$ 

$$A_1 k_{D1}^2 + A_2 k_{D1} + A_3 = 0$$
, and  $B_1 k_{D2} + B_2 k_{D1} + B_3 = 0$ , (3.10)

where  $A_1$ ,  $A_2$ ,  $A_3$ ,  $B_1$ ,  $B_2$ ,  $B_3$  are polynomials from  $\mathbb{Q}[T_1^{[i]}, T_2^{[i]}, X^{[i]} \mid i = 1, 2]$ . Furthermore,  $A_1$  and  $B_1$  factor as follows:

$$A_1 = X^{[1]}X^{[2]}(T_1^{[1]}X^{[2]} - T_1^{[2]}X^{[1]})(T_1^{[1]}T_2^{[1]}X^{[2]} - T_1^{[2]}T_2^{[2]}X^{[1]}), \tag{3.11a}$$

$$B_1 = T_1^{[1]} T_1^{[2]} (T_2^{[1]} X^{[2]} - T_2^{[2]} X^{[1]}). {(3.11b)}$$

Therefore,  $A_1$  and  $B_1$  will not vanish as long as the ratios  $\frac{X}{T_1}$ ,  $\frac{X}{T_2}$ ,  $\frac{X}{T_1T_2}$  are different in the first two experiments. Equations (3.6), (3.7), and (3.8) yield formulas for the steady state in terms of  $k_{D1}$ ,  $k_{D2}$ ,  $c_1$ ,  $c_2$ ,  $c_3$ . These formulas are substituted in  $\frac{X}{T_1}$ ,  $\frac{X}{T_2}$ ,  $\frac{X}{T_1T_2}$  to obtain three non-constant functions with respect to  $c_3$ . Therefore, outside of a set of measure zero,  $A_1$  and  $B_1$  will not vanish. Thus, (3.10) implies that generically, two experiments are sufficient to find  $k_{D1}$  and  $k_{D2}$  up to at most two options.

**Three experiments** For the three experiment case, since the projections above could be computed for the second and third experiment, not for the first and second, if  $T_1^{[1]}, T_2^{[1]}, X^{[1]}$  is substituted with  $T_1^{[3]}, T_2^{[3]}, X^{[3]}$  in the first equation in (3.10), there can be a true relation. This will yield one

more quadratic equation for  $k_{D1}$ , denoted by  $\widetilde{A}_1k_{D1}^2+\widetilde{A}_2k_{D1}+\widetilde{A}_3=0$ . If it is not proportional to the original equation, this will leave at most one value for  $k_{D1}$ . A sufficient condition for this non-proportionality would be  $A_1\widetilde{A}_3-\widetilde{A}_1A_3=0$ . To check this, one can plug again the formulas of the steady state in terms of  $k_{D1},k_{D2},c_1,c_2,c_3$  from (3.6), (3.7), and (3.8) and observe that  $A_1\widetilde{A}_3-\widetilde{A}_1A_3$  is a non-constant function in  $k_{D1},k_{D2},c_1,c_2,c_3^{[1]},c_3^{[2]},c_3^{[3]}$ . Therefore,  $A_1\widetilde{A}_3-\widetilde{A}_1A_3\neq 0$  outside of a set of measure zero. Therefore,  $k_{D1}$  and  $k_{D2}$  are generically uniquely identifiable from three experiments.

## 3.4 Optimal binding kinetics

In this part we investigate the basic characteristics of the bell-shape response, trimer concentration presented in Figure 3.2a, to have a better understanding of the optimal binding kinetics of a BiTE antibody at the site of action, e.g. TME. The maximum concentration of the trimer complex, peak of the bell shape, and its corresponding initial BiTE antibody condition are taken as the main characteristic values of the bell-shape. The first step is to visualize the sensitivity of the peak of the bell-shape to the dissociation rates of the binding kinetics of the BiTE antibody to its targets, and target concentrations. The parameters used in this section are based on the model represented in [56] for PF-06671008 BiTE antibody for solid tumors.

Figure 3.3 represents how change of dissociation rates and initial concentration of the targets affect the peak of the trimer concentration, and its corresponding BiTE antibody concentration. From the left side of figure 3.3a, sensitivity of the maximum trimer peak to the dissociation rates, it can be observed that an increase in dissociation rates  $k_{D1}$ , and  $k_{D2}$  significantly decrease the peak of the trimer concentration. On the other hand, by looking at the right side of figure 3.3a it can be observed that the optimal concentration of BiTE (the corresponding initial concentration of BiTE antibody at the peak of the trimer concentration) will be decreased by reducing the  $k_{D1}$  only, and increased by increasing either  $k_{D1}$  or  $k_{D2}$ . This result demonstrates that higher affinity, i.e. lower value of the dissociation rates, of the BiTE antibody is not effective in changing the maximum trimer concentration at the cite of action, i.g. in the TME. The sensitivity of the maximum trimer concentration, and optimal BiTE antibody initial concentration to the initial concentrations of the targets on the immune cells  $T_1(0)$ , and cancer cells  $T_2(0)$  is visualized in one dimensional plots of Figure 3.3b. From the left side, it can be observed that the maximum trimer concentration is sensitive to T1(0) and insensitive to T2(0), which physically makes sense since the initial concentration of the first target, CD3 receptors on the immune system, is much less than the second target, P-cad protein

on the tumor cells, in the TME. This results is consistent with the sensitivity analysis presented by [56]. Surprisingly, any change above 0.01x, or below 100x in the initial concentration of the target  $T_1(0)$  is not effective in changing optimal BiTE concentration, and significantly changes the optimal concentration BiTE antibody.

The dissociation rates  $k_{D1}$  and  $k_{D2}$  are dependent on the design of the BiTE antibody, while T1(0) and T2(0) are dependent on the tumor characteristics and variability among cancer patients. So, from the design perspective it would be ideal if the maximum trimer concentration and optimal BiTE concentration be less sensitive to the initial concentration of the targets. From the toxicity perspective, it would be favorable if a lower concentration of BiTE antibody can produce the same amount of trimer in the TME. In the one dimensional analysis presented in figure 3.3a, the optimal BiTE can be decreased as the dissociation rate of the first target  $k_{D1}$  becomes smaller, and it will result in a slightly higher trimer concentration that is favorable for efficacy.

Figure 3.4 extends the one dimensional visualizations presented in Figure 3.3 to two dimensions. The sensitivity of the maximum trimer concentration is on the left, and the sensitively of the corresponding initial concentration of the BiTE antibody is on the right side. The red color represents a higher value of the nM concentrations in log scale, and the blue color represents lower concentrations. The vertical pattern in Figure 3.4a, and the horizontal pattern in Figure 3.4d are consistent with the conclusions made from Figure 3.3. Moreover, the contrasting colors in the top left and the bottom right of Figure 3.4b suggest that a simultaneous increase in dissociation rates  $k_{D1}$ , with a decrease in  $k_{D2}$  is favorable in reducing the required concentration of BiTE antibody to achieved the peak of the trimer concentration. A cross check between Figures 3.4a, and 3.4b indicates that the simultaneous changes in  $k_{D1}$ , and  $k_{D2}$  to reduce the required trimer concentration to achieve the maximum concentration might not be favorable in increasing the maximum trimer concentration at the TME.

## 3.5 Comparison between BiTE antibodies

The presented three-body model 3.1 is used here to have a quantitative measure in comparing different CD3 BiTE antibody molecules presented in Table 3.1. The antibody molecules included in this study are designed for the two general categories of solid, and liquid tumors. Although each of the molecules might be different in the distribution, metabolism, and pharmacokinetics characteristics, the three-body model is what they all have in common at the cite of action. Beside the dissociation constants  $k_D$  values presented in Table 3.1, the initial concentration of the targets is

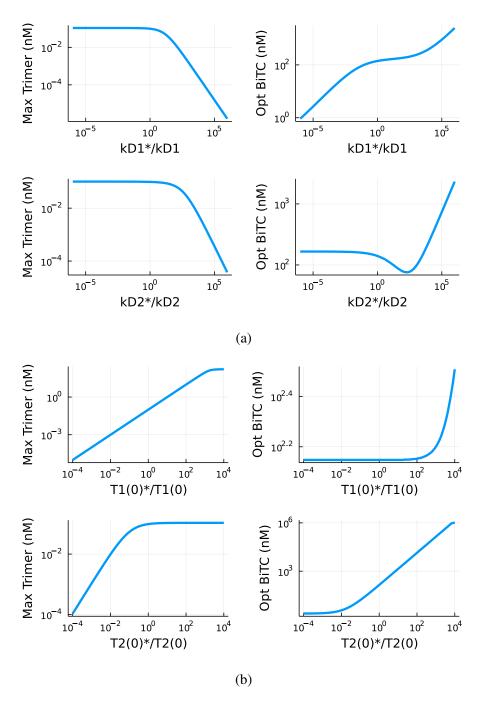


Figure 3.3: Log-log plots of bell-shape characteristics: the effects of (a) sweeping BiTE antibody dissociation rates to the targets and (b) sweeping target concentration in the TME on the optimal concentration of trimer and BiTE. The horizontal axes are log scale difference of the modified parameter (marked with a star\*) and its original value. Maximum trimer concentration is the peak of the bell-shape, and Optimal BiTE is the corresponding initial antibody concentration of the peak.

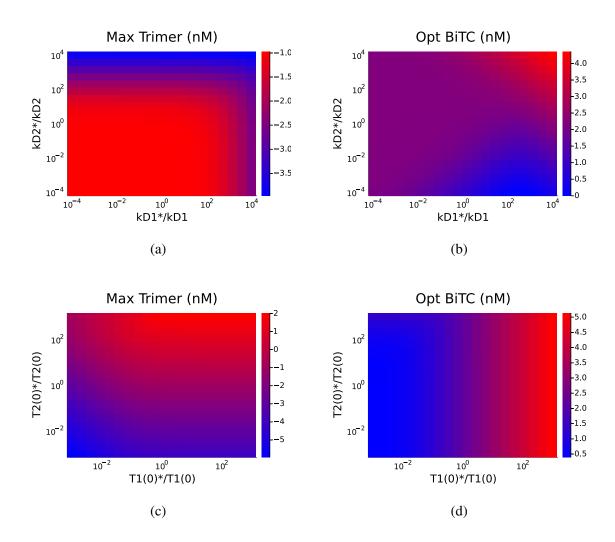


Figure 3.4: Bell-shape characteristics heatmap: the effects of sweeping the BiTE antibody dissociation rates,  $k_{D1}$  and  $k_{D2}$ , on (a) maximum of the trimer concentration of the bell-shape, and (b) corresponding, optimal, concentration of the BiTE antibody are represented on top. The effect of sweeping initial target concentrations to (c) the peak of bell-shape, and (d) optimal concentration of the antibody are presented on the bottom. The colors are plotted in log scale concentrations in nM. The horizontal and vertical axes are in log scale difference of the modified parameter (marked with a star\*) and its original value.

necessary for computational simulations of the three-body model. As the initial concentration of the target receptors is highly dependent of the cancer type and it might vary across different regions of the tumor, the comparison between the bell-shapes of BiTE molecules should be done for different initial concentrations of the targets.

A visual comparison between the bell-shapes of the molecules considered in this study is presented in Figure 3.5. The ratio of the initial concentration of the targets  $(T_1(0):T_2(0))$  are considered to be in the range of 1:10 to 1:1000 for solid tumors (Figure 3.5a), and in the range of 10:1 to 1:10 for liquid tumors (Figure 3.5b). It can be observed that in addition to the peak of the bell-shape, and the corresponding concentration of the BiTE antibody, the width of the bell-shape varies at different ratio of the initial concentration of the targets. For instance the width of the BiTE antibody Tarlatamab increases for dense tumor, where the initial concentration of the target proteins on cancer cells is much more than the target proteins on immune cells.

An analytic formulation of the basic characteristics of the bell-shape is done by [51]. The theoretical analysis has been done to understand the sensitivity of the peak of the bell-shape to binding kinetics of the bispecific antibody to each of the targets. Moreover, the with of the bell-shape could be approximated by initial concentrations of the targets at the cite of action. The presented results in this study is to have a quantitative comparisons between the BiTE molecules. For more theoretical understanding of the three-body problem, the readers are encouraged to the supplementary materials of [51].

The quantitative framework used for comparing bell-shapes of the BiTE antibody molecules at different ratios of initial concentration of the targets can be extended to continuous ratios of the targets. For this purpose, the basic characteristics of the bell-shape are extracted across different ratios between the targets, and represented in Figure 3.6. The peak of the trimer concentration is the maximum of bell-shape (on top), the corresponding BiTE concentration is the initial concentration of BiTE antibody that results in the maximum of the bell-shape (on middle), and the bell-shape width is simply the range of the BiTE antibody concentration that results in at least 50% of the maximum of the bell-shape (on bottom). For a realistic comparison between the BiTE antibodies design for solid tumors (Figure 3.6a), the left hand side of the horizontal axis should be considered, where the initial concentration of the target protein on cancer cells is much more that the initial concentration of the target protein CD3 on immune T cells. Similarly, for a realistic comparison between the BiTE antibodies designed for liquid tumors (Figure 3.6b), the right middle or right side of the horizontal should be taken into consideration.

From the three-body model perspective, a promising BiTE antibody is the one that creates

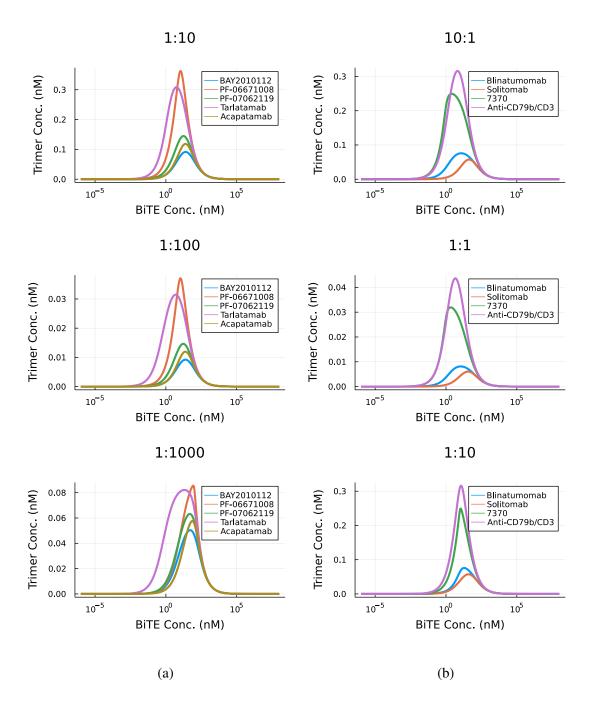


Figure 3.5: Numerical comparison between the bell shapes of BiTEs designed for (a) solid, and (b) liquid tumors. The relative concentration of the targets  $T_1(0):T_2(0)$  is printed on the top of each plot. The horizontal axes are in log scale, and the vertical axes are in linear scale.

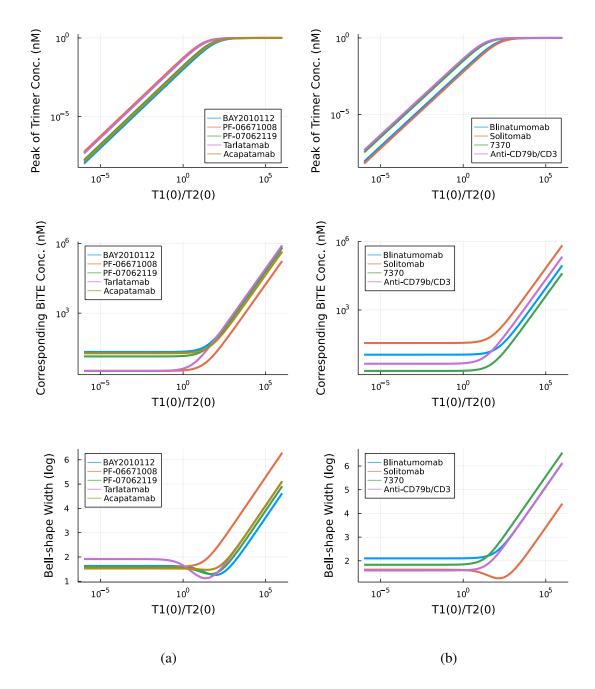


Figure 3.6: Numerical comparison between the basic characteristics of the bell-shape response of different BiTEs designed for (a) solid, and (b) liquid tumors. The top figure represent the value of the peak of bell-shape, the middle figures represent the corresponding BiTE antibody concentration at the peak of the bell-shape, and the bottom figures represent the width of the peak of the bell-shape. The relative initial concentration of the targets  $T_1(0)/T_2(0)$  is visualized in log scale of the horizontal axes.

the most trimer concentration with the minimal initial concentration of the antibody at the cite of action. Also, to overcome natural variability among different cancers and patients it is favorable to have a BiTE antibody with minimal variation for different ratios of the initial concentrations of the targets. So, A BiTE antibody molecule is effective at the cite of action if it results in: 1) a relatively higher peak of the trimer concentration, 2) a lower corresponding concentration of the BiTE at the peak of the trimer concentration, 3) a larger width of the bell-shape. Among the molecules presented in Figure 3.6, it can be observed the BiTE molecules like 7370, and PF-06671008 are outperforming in creating a large concentration of trimer concentration of tumor with minimal initial concentration. On the other hand, BiTEantibody molecule Solitomab, is creating a stable width of the peak for a wide range of ratios between the initial concentrations of the targets. It is apparent that, stability across different initial concentration of the targets increases the consistency of the data in clinical research.

## 3.6 Bio-distribution

A full dynamic model for BiTE for in human for Intravenous (IV) dose is introduced in [56]. A slightly different version of this model is used here as an starting point.

$$\dot{X}_{c} = \rho u(t) - k_{elD}X_{c} - k_{cp}X_{c} + k_{pc}X_{p}\frac{V_{p}}{V_{c}} - k_{cl}X_{c} - k_{lc}X_{l}\frac{V_{l}}{V_{c}} - k_{nl}X_{c}T_{lc} + k_{f1}D_{lc} - k_{n2}C_{c}T_{lc} + k_{f2}D_{lc} - k_{td}(X_{c} - \frac{X_{t}}{k_{c}})\frac{X_{1} + X_{2}}{wV_{c}}, \quad (3.12a)$$

$$\dot{X}_p = k_{cp} X_c \frac{V_c}{V_p} - k_{pc} X_p, \tag{3.12b}$$

$$\dot{X}_l = k_{cl} X_c \frac{V_c}{V_l} - k_{lc} X_l, \tag{3.12c}$$

$$T\dot{1}_c = -k_{ct}T T 1_c + k_{tc}T T 1_t \frac{M_1 + M_2}{wV_c} - k_{n1}X_c T 1_c - k_{f1}D 1_c, \tag{3.12d}$$

$$\dot{D1}_c = k_{n1} X_c T1_c - k_{f1} D1_c, \tag{3.12e}$$

$$\dot{T}_{c}^{2} = k_{syn} - k_{deq}T_{c}^{2} - k_{n2}X_{c}T_{c}^{2} + k_{f2}D_{c}^{2},$$
(3.12f)

$$\dot{D2}_c = -k_{elD} * D2_c + k_{n2} X_c T2_c - k_{f2} D2_c, \tag{3.12g}$$

$$\dot{X}_t = k_{td}(X_c - \frac{X_t}{k_{\varepsilon}}) - k_{n1}T1_tX_t - k_{n2}T2_tX_t + k_{f1}D1_t + k_{f2}D2_t, \tag{3.12h}$$

$$\dot{T1}_t = k_{ctT}T1_c \frac{wV_c}{M_1 + M_2} - k_{tcT}T1_t - k_{n1}T1_tC_t + k_{f1}D1_t - k_{n1}T1_tD2_t + k_{f1}Y, \quad (3.12i)$$

$$T\dot{2}_t = -k_{n2}T2_tC_t + k_{f2}D2_t - k_{n2}T2_tD1_t + k_{f2}Y, (3.12j)$$

$$\dot{D1}_c = k_{n1}C_cT1_c - k_{f1}D1_c \tag{3.12k}$$

$$\dot{D1}_t = k_{n1}T1_tC_t - k_{f1}D1_t - k_{n2}T2_tD1_t + k_{f2}Y, \tag{3.121}$$

$$\dot{D2}_t = k_{n2}T2_tC_t + k_{f2}D2_t - k_{n1}T1_tD2_t + k_{f1}Y, \tag{3.12m}$$

$$\dot{Y} = k_{n1}T1_tD2_t + k_{n2}T2_tD1_t - (k_{f1} + k_{f2})Y, \tag{3.12n}$$

$$\dot{M}_{1} = \frac{k_{ge}M_{1}(1 - \frac{M_{1} + M_{2}}{k_{v}})}{(1 + (\frac{k_{ge}}{k_{ol}}(M_{1} + M_{2}))^{k_{\psi}})^{1/k_{\psi}}} - \frac{k_{max} \times Y}{kc_{50} + Y}M_{1},$$
(3.12o)

$$\dot{M}_2 = \frac{k_{max} \times Y}{kc_{50} + Y} M_1 - M_2/k_{\tau}. \tag{3.12p}$$

Where X is the concentration of drug, T is the concentration of targets, D is the drug-target dimer concentration, Y is the trimer concentration, and M is the tumor volume intermediate compartment. All parameters and variables are defined in details in tables 3.2 and 3.3. The dot sign on top of the variables is a time derivative  $\dot{f}(t) = \frac{df(t)}{dt}$ . The differences between model 3.12 and the model presented in [56] are: 1) an extra medium for representing tissues with high concentration of immune cells, e.g. lymph nodes, 2) integrating tumor intermediate compartments into the other modules of the model, and 3) lower number of tumor intermediate compartments for representing the delay.

Table 3.2: Parameters used in model (3.12).

	Value	Unit	Definition
$V_c$	40.2	mL/kg	Volume of distribution in the central compartment
$\Lambda_p$	211	mL/kg	Volume of distribution in the peripheral compartment
$V_l$	92	mL/kg	Volume of distribution in the lymph compartment
$k_{el_D}$	$1.16\times10^{-1}$	1/h	Elimination rate of antibody in the central compartment
$k_{el_T}$	2.51	1/day	Elimination rate of immune cells (Target 1)
$k_{cp_D}$	$6.27\times10^{-1}$	1/h	Antibody redistribution to the peripheral compartment
$k_{pc_D}$	$1.19\times10^{-1}$	1/h	Antibody redistribution to the central compartment
$k_{ct_T}$	$2 \times 10^{-3}$	1/day	T cell (target 1) redistribution to the TME
$k_{tc_T}$	$5 \times 10^{-4}$	1/day	T cell (target 1) redistribution to the central compartment
$k_{n_1}$	1.72	1/nM/h	Binding of the antibody and target 1
$k_{f_1}$	19.66	1/h	Unbinding rate of the antibody-target 2 dimer
$k_{n_2}$	1.57	1/nM/h	Binding rate of the antibody and target 2
$k_{f_2}$	0.74	1/h	Unbinding rate of the antibody-target 2 dimer
$k_{deg}$	$1.5\times10^{-1}$	1/h	Tumor $T2_c$ degradation rate
$k_{syn}$	$k_{deg} \times T2_c(0)$	1/h	Tumor synthesis rate (assuming no proliferating tumor)
$k_{ctT}$	$2 \times 10^{-3}$	1/day	T cell redistribution from the central to the TME
$k_{tcT}$	$5 \times 10^{-4}$	1/day	T cell redistribution from the TME.
$k_{max}$	1.32	1/day	Maximum killing rate
$kc_{50}$	$6.9 \times 10^{-5}$	Мп	Concentration at half maximum
$k_{ge}$	$1.9\times10^{-1}$	1/day	Exponential tumor growth rate
$k_{gl}$	$1.23\times10^{-1}$	mL/day	Linear tumor growth rate
$k_v$	0.9	mL	Maximum tumor volume
$k_{ au}$	3.99	day	Transduction time between tumor compartments.
$k_{\psi}$	20	1	Exponential to linear transition rate of the tumor
m	09	kg	Weight of a patient.
θ	9.52	${ m nM/}(\mu{ m g/kg})$	Drug conc. in the central compartment for $1\mu g/kg$ dose

Table 3.3: Variables used in model (3.12).

Variable Unit	Unit	Initial value	Definition
n	mg/kg/day	1	Input: drug dose.
$X_c$	nM	0.0	Antibody concentration in central compartment.
$X_p$	nM	0.0	Antibody concentrations in peripheral compartment.
$X_t^{\cdot}$	nM	0.0	Antibody concentrations in the TME.
$T1_c$	nM	0.83	Target 1 concentration in the central compartment.
$T1_t$	nM	$1.08\times10^{-1}$	Target 1 concentration in the TME.
$T2_c$	nM	1.1	Target 2 concentration in the central compartment.
$T2_t$	nM	$1.66 \times 10^2$	Target 2 concentration in the TME.
$D1_c$	nM	0.0	Dimer drug-target 1 in the central compartment.
$D1_t$	nM	0.0	Dimer drug-target 1 in the TME.
$D2_c$	nM	0.0	Dimer drug-target 2 in the central compartment.
$D2_t$	nM	0.0	Dimer drug-target 2 in the TME.
$\lambda$	nM	0.0	Trimer concentration in the TME.
M1	mL	1.0	Tumor volume in growth compartment.
M2	mL	0.0	Tumor transduction compartment.

## **Computational resources**

SIAN [71] is used for structural identifiability analysis, and analytical derivations. Numerical simulations and figures are produced with Julia programming language [73]. DifferentialEquations package is used numerical calculations [74]. The numerical software for reproducing the figures presented in the manuscript along with more examples is available at https://github.com/mahdiarsadeghi/bites.

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## **Chapter 4**

# **Epidemics**

COVID-19, a highly contagious disease, has been spreading between continents and has already claimed more than 2.5 million lives globally during its first year [75], and has resulted in a worldwide economic downturn [76]. Unsurprisingly, this has sparked a renewed interest in the dynamical modeling and analysis of infectious diseases, particularly in the control theory and dynamical systems communities [77–85].

There has been much recent theoretical work revisiting, expanding, and studying dynamical and control properties of classical epidemic models so as to understand the spread of COVID-19 during quarantine and social distancing [86–91], including studies of (integral) input to state stability [92], network stability of epidemic spread [93, 94], and optimal control strategies for meta-population models [95]. These models have been used to predict the potential number of infected individuals and virus-related deaths, as well as to aid government agencies in decision making [96]. Most models are variations on the classical *SIR* model [97–99] which have been modified to more closely predict the spread of COVID-19. Some such extensions are listed below:

- Expanding the SIR model to include additional population compartments. Such compartments
  may describe individuals that are placed under quarantine and/or in social isolation. Other
  models explicitly subdivide populations into both symptomatic and asymptomatic infected
  individuals [100–105], as it is currently thought that COVID-19 is significantly spread through
  asymptomatic individuals [106–108].
- 2. Modeling the effects of social distancing for an infection aware population. This can be done by changing the contact rates between the compartments, or by modeling the behavior of a

#### CHAPTER 4. EPIDEMICS

population that alters its social interactions because of observed infections or deaths [109, 110]. The latter technique has recently been applied to COVID-19 [111, 112].

3. Sub-dividing populations into regions, each described by *local* parameters. Such regions may be cities, neighborhoods, or communities [113]. This framework allows modelers to capture the virus spread and population mobility geographically [114–117]. These models have been recently used to understand the spread of COVID-19 in China [118], Italy [119], Netherlands and Belgium [120], and India [121, 122].

Shortening the period of time that populations are socially distanced is economically advantageous [76, 123, 124]. The main objective of this study is to reduce the disease burden (here measured as the peak of the infected population) while simultaneously minimizing the length of time that the population is socially distanced.

The starting point in modern epidemiological modeling is the Kermack-McKendrick model [97, 125] which is known as the Susceptible-Infectious-Removed (SIR) model. It assumes a well-mixed homogeneous population, and it can be written as the three-compartment model:

$$\dot{S}(t) = -c\beta S(t)I(t),$$

$$\dot{I}(t) = c\beta S(t)I(t) - \gamma I(t),$$

$$\dot{R}(t) = \gamma I(t),$$
(4.1)

where S(t), I(t), R(t) refer to the susceptible, infective, and removed individuals at time t. The product  $b = c\beta$  and the parameter  $\gamma$  are called the *infection rate* and the *removal rate*, respectively. We factored the infection rate as  $b = c\beta$ , where we call c and  $\beta$  the *intrinsic infection rate* and the *contact rate* respectively, to emphasize that b depends on both *biological* and *societal* conditions.

## 4.1 Optimal timing

Social Distancing (SD) as a form of NPI has been enacted in many countries as a form of mitigating the spread of COVID-19. There has been a large interest in mathematical modeling to aid in the prediction of both the total infected population and virus-related deaths, as well as to aid government agencies in decision making. As the virus continues to spread, there are both economic and sociological incentives to minimize time spent with strict distancing mandates enforced, and/or to adopt periodically relaxed distancing protocols, which allow for scheduled economic activity. The

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main objective of this section is to reduce the disease burden in a population, here measured as the peak of the infected population, while simultaneously minimizing the length of time the population is socially distanced, utilizing both a single period of social distancing as well as periodic relaxation. A linear relationship is derived among the optimal start time and duration of a single interval of social distancing from an approximation of the classic epidemic SIR model. Furthermore, there is a sharp phase transition region in start times for a single pulse of distancing, where the peak of the infected population changes rapidly; notably, this transition occurs well before one would intuitively expect. By numerical investigation of more sophisticated epidemiological models designed specifically to describe the COVID-19 pandemic, we see that all share remarkably similar dynamic characteristics when contact rates are subject to periodic or one-shot changes, and hence lead us to conclude that these features are universal in epidemic models. On the other hand, the nonlinearity of epidemic models leads to non-monotone behavior of the peak of infected population under periodic relaxation of social distancing policies. This observation led to hypothesize that an additional single interval social distancing at a proper time can significantly decrease the infected peak of periodic policies, and verified numerically. While synchronous quarantine and social distancing mandates across populations effectively minimize the spread of an epidemic over the world, relaxation decisions should not be enacted at the same time for different populations.

After the shelter-in-place ordinances [126], social distancing as a form of NPI has been enacted in the United States [127], and other countries [128, 129] for reducing the spread of the virus, as neither herd immunity nor a viable vaccine yet existed [130]. Many countries have implemented strict quarantine, isolation, or social distancing policies early in the epidemic [128], while countries such as Belarus [131] and Sweden [132, 133] have taken more lenient approaches at the onset of the outbreak. Understanding optimal strategies for social distancing will both "flatten the curve" and hopefully ease the economic burden experienced due to prolonged economic stagnation [134–136]. The goal of this section is thus to investigate the response of the disease to different time-varying social distancing strategies.

## 4.2 Singular purterbation approach

In order to control highly-contagious and prolonged outbreaks, public health authorities intervene to institute social distancing, lock-down policies, and other NPIs. Given the high social, educational, psychological, and economic costs of NPIs, authorities tune them, alternatively tightening up or relaxing rules, with the result that, in effect, a relatively flat infection rate results.

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For example, during the summer in parts of the United States, daily COVID-19 infection numbers dropped to a plateau. This paper approaches NPI tuning as a control-theoretic problem, starting from a simple dynamic model for social distancing based on the classical SIR epidemics model. Using a singular-perturbation approach, the plateau becomes a Quasi Steady State (QSS) of a reduced two-dimensional SIR model regulated by adaptive dynamic feedback. It is shown that the QSS can be assigned and it is globally asymptotically stable. Interestingly, the dynamic model for social distancing can be interpreted as a nonlinear integral controller. Problems of data fitting and parameter identifiability are also studied for this model. The paper also discusses how this simple model allows for a meaningful study of the effect of population size, vaccinations, and the emergence of second waves.

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# Appendix A

# **First Appendix Headline**

# **Appendix B**

# **Second Appendix Headline**