

Assignment 5

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Biomedical Signal and Image Processing Lab

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Frequency Band Limitation and Noise Reduction of Signal

In this section, we explore methods to limit the frequency band of an ECG signal and reduce noise by applying various filtering techniques. The data used in this experiment is from a healthy volunteer, sampled at 250 Hz and saved in normal.mat with two columns representing time (in seconds) and the ECG signal (in volts).

— Question 1

Analyze a typical 10-second segment from the clean ECG data in terms of frequency content using the pwelch function. Similarly, select a 10-second segment from the noisy data and examine its frequency content as well. Plot the power spectrum in dB for both segments, paying attention to the frequency content of the noisy and clean signals.

```
1
       %% Section 1
 2
       clc; close all;
 3
 4
       load('normal.mat');
 5
 6
       % Parameters
 7
       Fs = 250;
 8
       t = normal(:,1);
9
       t_total = length(sig) / Fs;
10
       sig = normal(:,2);
       sig2 = randn(1,1000);
11
12
13
       %% Q1.1
14
       % Time segments for clean and noisy parts
15
       t_clean_start = 5;
16
       t_clean_end = 15;
17
       t_noisy_start = 250;
18
       t_noisy_end = 260;
19
20
       % Clean and noisy signal segments
21
       sig_clean = sig(t_clean_start*Fs+1 : t_clean_end*Fs);
22
       sig_noisy = sig(t_noisy_start*Fs+1 : t_noisy_end*Fs);
23
24
       % Clean signal segment
25
       figure;
       subplot(2, 2, 1);
26
27
       plot(t(t_clean_start*Fs+1 : t_clean_end*Fs), sig_clean);
28
       title('Clean Signal Segment');
29
       xlabel('Time (s)');
30
       ylabel('Amplitude (V)');
31
32
       % Noisy signal segment
33
       subplot(2, 2, 2);
       plot(t(t_noisy_start*Fs+1 : t_noisy_end*Fs), sig_noisy);
34
35
       title('Noisy Signal Segment');
       xlabel('Time (s)');
36
37
       ylabel('Amplitude (V)');
38
39
       % PSD for clean signal segment
40
       subplot(2, 2, 3);
41
       window = gausswin(128);
42
       noverlap = 64;
       nfft = 128;
43
```

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```
44
       [p,f] = pwelch(sig_clean', window, noverlap, nfft, Fs);
45
       plot(f,db(p))
46
       title('Power Spectrum of Clean Signal Segment');
47
       xlabel('Frequency (Hz)');
48
       ylabel('Power/Frequency (dB/Hz)');
49
       xlim([0,120]);
50
51
       % PSD for noisy signal segment
52
       subplot(2, 2, 4);
53
       [p, f] = pwelch(sig_noisy', window, noverlap, nfft, Fs);
54
       plot(f,db(p))
55
       title('Power Spectrum of Noisy Signal Segment');
56
       xlabel('Frequency (Hz)');
57
       ylabel('Power/Frequency (dB/Hz)');
58
       xlim([0,120]);
```

Source Code 1: Frequency Analysis of Clean and Noisy ECG Segments

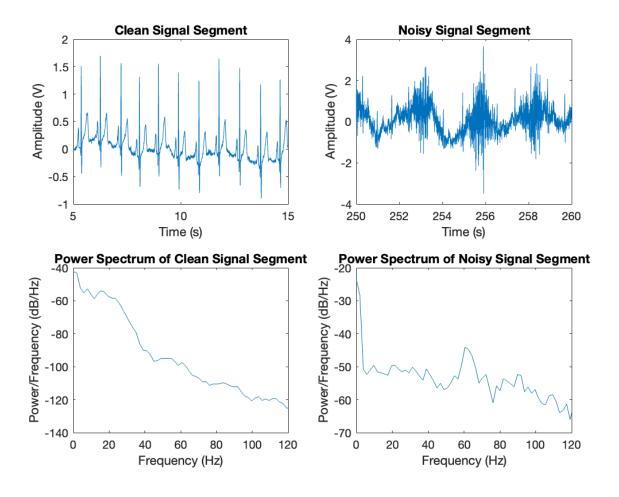


Figure 1: Power Spectral Density of Signals

Upon analyzing the noisy segment of the signal, it appears that EMG artifacts have affected the ECG signal. Additionally, observing the frequency domain, we can see that the noisy segment contains more energy in the higher frequencies.

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— Question 2

Design a bandpass filter for frequency limitation of the signal. The filter should remove baseline fluctuations and reduce high-frequency noise while preserving energy within the main frequency range of the signal. Avoid sharp transition bands when selecting the filter's lower and upper cutoff frequencies. Use the plot function instead of stem to display the impulse response of the filter.

```
1
      %% Q1.2
2
       n = size(normal, 1);
3
4
       % Frequency limits
5
       low_freq = 1 * n / Fs;
       high\_freq = 90 * n / Fs;
6
7
8
      % FFT of the signal and isolate positive frequencies
9
       normal_fft = abs(fftshift(fft(normal(:, 2))));
10
       normal_half = normal_fft(n/2+1:n);
11
12
       % Power of the signal
13
       normal_pwr = sum(normal_half(low_freq:n/2).^2);
14
15
       \% Bandstop filter to attenuate frequencies between 1 and 90 Hz
16
       [b, a] = butter(3, [1/(Fs/2) \ 40/(Fs/2)], 'stop');
17
       normal_filtered = filter(b, a, normal_half(low_freq:n/2));
18
19
       % Power of the filtered signal
20
       filter_pwr = sum(normal_filtered.^2);
21
22
       % Frequency response of the filter
23
       figure;
24
       subplot(2, 1, 1);
25
       freqz(b, a, 50);
26
       title("Frequency Response of Bandstop Filter");
27
       grid minor;
28
29
       % Impulse response of the filter
30
       subplot(2, 1, 2);
31
       impz(b, a, 50);
32
       title("Impulse Response of Bandstop Filter");
33
       grid minor;
```

Source Code 2: Bandpass Filter Design and Impulse Response

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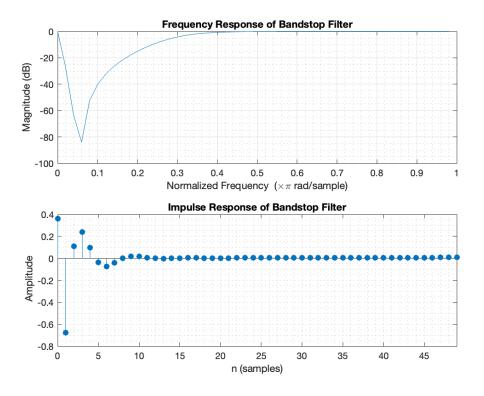


Figure 2: Frequency and Impulse Responses of the Designed Bandstop Filter

To design a filter with a linear phase response and avoid phase distortion, we use an FIR filter. This filter is designed using the filterDesigner tool in MATLAB.

— Question 3

Filter the designed segments (each 10-second segment) of the clean and noisy ECG data, and show how much noise is removed by the filter by plotting the power spectrum of the filtered signal.

```
1
       %% Q1.3
2
       % Filter the clean and noisy segments
3
       clean_filtered = filter(b, a, clean_signal);
4
       noisy_filtered = filter(b, a, noisy_signal);
5
6
       figure;
7
       % PSD of filtered clean signal
8
       subplot(2, 1, 1);
9
       [p, f] = pwelch(clean_filtered', [], [], Fs);
10
       plot(f,db(p))
11
       title("Clean ECG Signal (Filtered)");
12
       grid minor;
13
       xlim([0 120]);
14
       % PSD of filtered noisy signal
15
       subplot(2, 1, 2);
16
       [p, f] = pwelch(noisy_filtered', [], [], Fs);
17
       plot(f,db(p))
18
       title("Noisy Signal (Filtered)");
19
       grid minor;
20
       xlim([0 120]);
```

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Source Code 3: Evaluation of Filtered Signal Segments

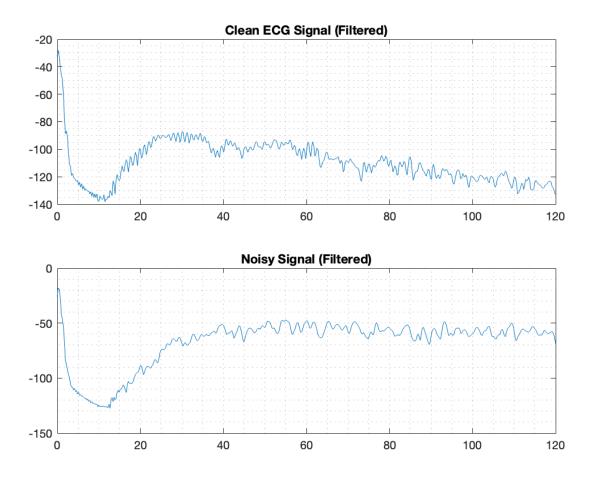


Figure 3: Power Spectral Density of Filtered Clean and Noisy ECG Signals

Soloution

Based on the plots, we observe that the designed filter performs effectively in removing noise from the signal. Both filtered outputs display similar patterns, indicating that the filter successfully attenuated unwanted noise components.

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Detection of Cardiac Arrhythmias

In this section, a system is designed for detecting abnormal cardiac arrhythmias. Non-normal ECG segments are taken from the MIT-BIH arrhythmia database, recorded in a hospital setting. The dataset contains 10-minute recordings sampled at 250 Hz with 12-bit quantization.

lacksquare Question 1

To design the detection system, certain criteria must be established to distinguish between normal and abnormal ECGs. Select a few files from the list below and load them in MATLAB to read and plot the ECG signals. Identify which segment corresponds to normal or abnormal (arrhythmic) signals for each pair and analyze their frequency content using the 'pwelch' function. Compare the normal and arrhythmic segments and note observations for identifying arrhythmias.

- n_422.mat episode of ventricular fibrillation
- n 424.mat episode of ventricular fibrillation
- n_426.mat ventricular fibrillation and low frequency noise
- n 429.mat ventricular flutter (2 episodes) and ventricular tachycardia
- n 430.mat ventricular flutter and ventricular fibrillation
- n_421.mat normal sinus rhythm with noise
- n 423.mat atrial fibrillation and noise

```
%% 2-1
1
2
       load("n_422.mat");
3
       fs = 250;
4
5
       normal_1=n_422(8210:10710);
6
       abnormal_1=n_422(11442:13942);
7
8
       normal_2=n_422(1:2500);
9
       abnormal_2=n_422(57211:59711);
10
11
       t_normal_1=0:1/fs:length(normal_1)/fs-1/fs;
12
       t_abnormal_1=0:1/fs:length(abnormal_1)/fs-1/fs;
13
14
       t_normal_2=0:1/fs:length(normal_2)/fs-1/fs;
15
       t_abnormal_2=0:1/fs:length(abnormal_2)/fs-1/fs;
16
17
18
       subplot (4,1,1)
19
       pwelch(normal_1)
20
       title("normal 1")
21
       subplot (4,1,2)
22
       pwelch(abnormal_1)
23
       title("abnormal 1")
24
       subplot (4,1,3)
25
       pwelch(normal_2)
26
       title("normal 2")
27
       subplot (4,1,4)
28
       pwelch(abnormal_2)
```

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```
29 title("abnormal 2")
```

Source Code 4: Classification Criteria for Normal and Abnormal ECG

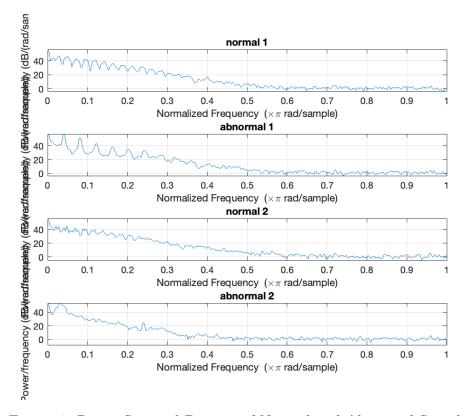


Figure 4: Power Spectral Density of Normal and Abnormal Signals

The abnormal ECG signal has more energy at higher frequencies.

— Question 2

Identify the differences between normal and arrhythmic segments in both time and frequency domains. Use appropriate plots to compare these differences.

```
% 2-2
1
2
       figure
3
       subplot(2,1,1)
4
       plot(t_normal_1, normal_1);
       xlabel('time(second)')
5
       title("normal 1")
6
7
       subplot (2,1,2)
       plot(t_abnormal_1,abnormal_1);
8
9
       xlabel('time(second)')
10
       title("abnormal 1")
11
12
       figure
13
       subplot(2,1,1)
14
       plot(t_normal_2, normal_2);
15
       xlabel('time(second)')
16
       title("normal 2")
17
       subplot(2,1,2)
```

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```
plot(t_abnormal_2,abnormal_2);
    xlabel('time(second)')
    title("abnormal 2")
```

Source Code 5: Differences between Normal and Arrhythmic Segments

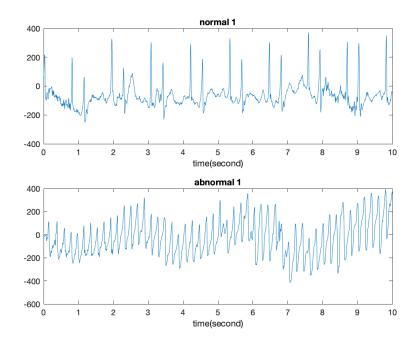


Figure 5: Segmentation of first Normal and Abnormal Signals

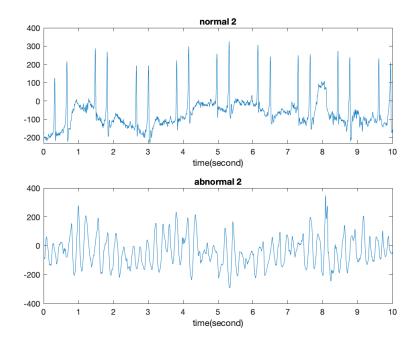


Figure 6: Segmentation of second Normal and Abnormal Signals

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In the arrhythmic time domain, there is no distinct regular pattern or rhythm. In the frequency domain, there is also higher energy at the high frequencies in the arrhythmic segments.

$lue{}$ Question 3

Label each signal segment using predefined windows for different time frames and assign real labels to evaluate performance. Use 5-second windows with a 50% overlap and label each window as per the provided standards.

Assign labels for each window as follows:

- 1. 1: Normal
- 2. 2: VFIB (Ventricular Fibrillation)
- 3. 3: VT (Ventricular Tachycardia)
- 4. 4: Noise
- 5. 0: None

```
%% 2-3
 1
 2
       labels=zeros(59,11);
 3
       for i=1:59
 4
            t_start=(i-1)*5*250;
 5
            t end=((i-1)*5+10)*250;
 6
            labels(i,2)=t_end;
 7
            if((t_start>=1 && t_end<10711))</pre>
 8
                 labels(i,1)=1;
9
            elseif((t_start>=10711 && t_end<11211))</pre>
10
                 labels(i,1) = 3;
            elseif((t_start>=11211 && t_end<11441))</pre>
11
12
                 labels(i,1) = 1;
13
            elseif((t_start>=11442 && t_end<59711))</pre>
14
                 labels(i,1) = 3;
15
            elseif((t_start>=59711 && t_end<61288))</pre>
16
                 labels(i,1)= 4;
17
            elseif((t_start>=61289))
18
                 labels(i,1) = 2;
19
20
                 labels(i,1) = 0;
21
            end
22
       end
```

Source Code 6: Labeling of Signal Windows

— Question 4

For classifying the VFIB and Normal windows in the n_422.mat signal, examine frequency-based features within these windows. Use different features (e.g., bandpower, medfreq, mean-freq) to analyze and select distinguishing characteristics.

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```
4
       for i=1:59
5
           if(labels(i,1)==1 || labels(i,1)==2)
               signal = n_422(labels(i,2)-10*250+1:labels(i,2));
6
7
               filtered_signal=filtfilt(d, signal);
8
               labels(i,3)=meanfreq(signal);
9
               labels(i,4)=medfreq(signal);
10
               labels(i,5)=sum(filtered_signal.^2,'all');
11
           end
12
       end
13
14
       normal features=labels(2:7,:);
15
       VFIB_features=labels(51:59,:);
```

Source Code 7: Frequency-Based Feature Extraction and Classification

— Question 5

Calculate morphological (time-domain shape) and statistical features for the VFIB and Normal windows. Select various features for all windows, including max, min, peak-to-peak, number of zero crossings, and variance. Plot the histograms of features for both VFIB and Normal windows and compare them to evaluate feature separability.

```
%% 2-5
1
2
       figure
3
      histogram(normal_features(:,3).','FaceColor', 'blue','BinWidth',0.005)
4
5
       histogram(VFIB_features(:,3),'FaceColor', 'red','BinWidth',0.005)
6
       legend("normal","VFIB")
7
       title("mean frequency")
8
       hold off
9
10
       figure
11
      histogram(normal_features(:,4).','FaceColor', 'blue','BinWidth',0.005)
12
       histogram(VFIB_features(:,4),'FaceColor', 'red','BinWidth',0.005)
13
14
       legend("normal","VFIB")
15
       title("median frequency")
16
       hold off
17
18
       figure
19
       histogram(normal_features(:,5).','FaceColor', 'blue','BinWidth',10^5)
20
21
       histogram(VFIB_features(:,5), 'FaceColor', 'red', 'BinWidth',10^5)
22
       legend("normal","VFIB")
23
       title("band power")
24
       hold off
```

Source Code 8: Morphological and Statistical Feature Calculation

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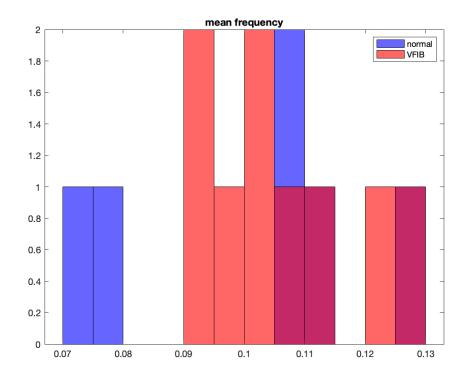


Figure 7: Mean Frequency Comparison for Normal and VFIB Segments

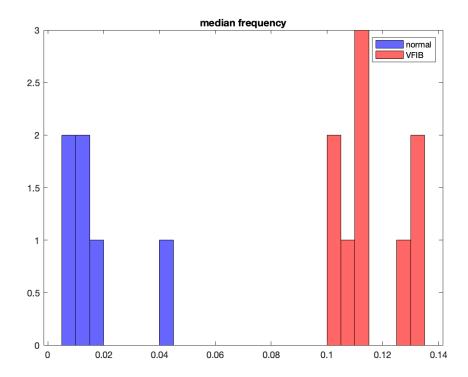


Figure 8: Median Frequency Comparison for Normal and VFIB Segments

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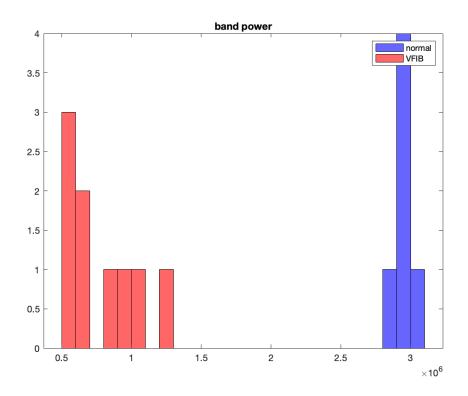


Figure 9: Delta Power in 10-30 Hz Band Comparison for Normal and VFIB Segments

Observations from the feature comparison:

- Criterion 1: Mean frequency is not suitable for accurate classification.
- Criterion 2: Median frequency is suitable for classification, with a threshold set at approximately 0.07.
- Criterion 3: Power in the 10 to 30 Hz band is suitable for classification, with a threshold set at approximately 2×10^6 .

$lue{}$ Question 6

Considering the results of previous part, choose two features and, for each one, complete the function va_detect.m. Obtain and review the alarm vector (output detected by the feature). Windowing in the function va_detect.m is similar to the implementation in question 2, and the alarm vector is similar to the actual labels in question 3.

```
[alarm_bandpower,t_bandpower] = va_detect(n_422 , fs, 'bansdpower');
[alarm_med,t_med] = va_detect(n_422 ,fs ,'med');
```

Source Code 9: Histogram Comparison of VFIB and Normal Features

— Question 7

For each of the features in previous question, form a *Confusion* matrix (two classes, considering VFIB as positive and Normal as negative) and calculate the metrics *Sensitivity*, *Specificity*, and *Accuracy*. For the windows that are labeled neither VFIB nor Normal, what was the diagnostic outcome?

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```
%% 2-7
1
      targets = labels((labels(:,1) == 1 | labels(:,1) == 2) , 1) == 2;
2
3
      outputs_med = alarm_med((labels(:,1) == 1 | labels(:,1) == 2)) == 1;
4
      outputs_bp = alarm_bandpower((labels(:,1) == 1 | labels(:,1) == 2)) == 1;
5
6
      cm1 = confusionmat(targets, outputs_bp);
7
      confusionchart(cm1)
8
9
      cm2 = confusionmat(targets, outputs_med);
10
      confusionchart(cm2)
```

Source Code 10: Confusion Matrix and Performance Metrics Calculation

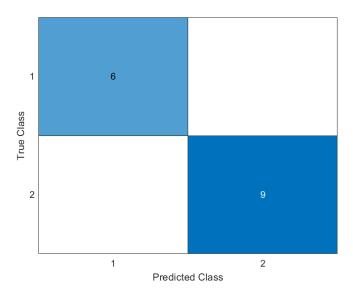


Figure 10: Two class classification based on Band Power confusion matrix

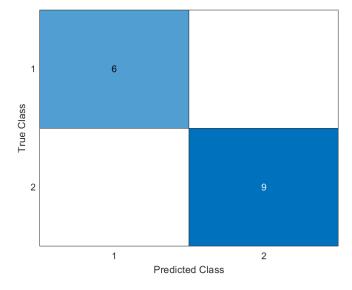


Figure 11: Two class classification based on Median Frequency confusion matrix

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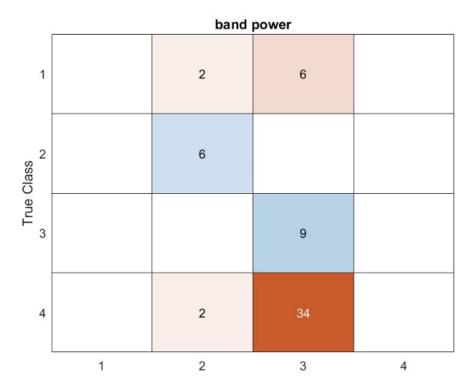


Figure 12: 4 class classification based on Band Power confusion matrix

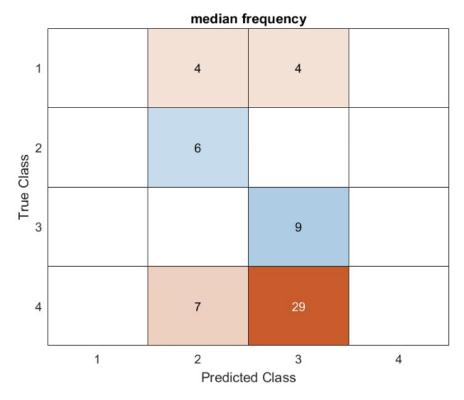


Figure 13: 4 class classification based on Median Frequency confusion matrix

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Two-Class Classification Based on Band Power and Median Frequency

- Accuracy = $\frac{6+9}{6+9+0+0} = 1.0$
- Sensitivity = $\frac{6}{6+0} = 1.0$
- Specificity = $\frac{9}{9+0} = 1.0$

four-Class Classification Based on Band Power:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 2 to 6.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 2 to 34.

four-Class Classification Based on Median Frequency:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 4 to 4.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 7 to 29.

Question 8

In this section, we aim to evaluate the effectiveness of morphological (shape-temporal) and statistical features in classifying VFIB and normal windows. We examine various morphological and statistical features and select a few to compute for all data windows. You may use the following features:

- Maximum amplitude (max)
- Minimum amplitude (min)
- Peak-to-peak amplitude (peak-to-peak)
- Use the findpeaks command to determine local maxima and minima and use it to compute the mean R-peak amplitude.
- Number of zero crossings
- Variance of amplitudes (var)

```
1
      for i=1:59
2
           if(labels(i,1)==1 || labels(i,1)==2)
3
               signal = n_422(labels(i,2)-10*250+1:labels(i,2));
               labels(i,6)=min(signal);
4
5
               labels(i,7)=max(signal);
6
               labels(i,8)=labels(i,7)-labels(i,6);
7
               labels(i,9)=mean(findpeaks(signal),'all');
8
               labels(i,10)=sum(signal==0);
9
               labels(i,11)=var(signal);
10
```

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```
11 end

12

13 normal_features=labels(2:7,[6:11]);

14 VFIB_features=labels(51:59,[6:11]);
```

lacksquare Question 9

For each of the computed features in previous question, plot the histogram (using the hist command) of the feature for the two classes, VFIB and Normal, and compare them. Is it possible to separate the two classes using this feature? Select a threshold for each feature to classify the two classes.

```
1
       figure
 2
 3
       histogram(normal_features(:,1), 'FaceColor', 'blue', 'BinWidth',20)
4
       histogram(VFIB_features(:,1),'FaceColor', 'red','BinWidth',20)
 5
       legend("normal","VFIB")
 6
 7
       title("min amplitude")
 8
       hold off
9
10
       figure
11
12
       histogram(normal_features(:,2), 'FaceColor', 'blue', 'BinWidth',30)
13
14
       histogram(VFIB_features(:,2), 'FaceColor', 'red', 'BinWidth',30)
       legend("normal","VFIB")
15
       title("max amplitude")
16
17
       hold off
18
19
       figure
20
21
       histogram(normal_features(:,3).','FaceColor', 'blue','BinWidth',30)
22
23
       histogram(VFIB_features(:,3),'FaceColor', 'red','BinWidth',30)
       legend("normal","VFIB")
24
25
       title("peak to peak")
26
       hold off
27
28
       figure
29
30
       histogram(normal_features(:,4).','FaceColor', 'blue','BinWidth',8)
31
       hold on
32
       histogram(VFIB_features(:,4), 'FaceColor', 'red', 'BinWidth',8)
33
       legend("normal","VFIB")
       title("mean R")
34
       hold off
35
36
37
       figure
38
39
       histogram(normal_features(:,5).','FaceColor', 'blue','BinWidth',3)
40
       hold on
41
       histogram(VFIB_features(:,5), 'FaceColor', 'red', 'BinWidth',3)
42
       legend("normal","VFIB")
43
       title("zero crossing")
       hold off
44
45
46
       figure
```

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```
histogram(normal_features(:,6).','FaceColor', 'blue','BinWidth',10^3)
hold on
histogram(VFIB_features(:,6),'FaceColor', 'red','BinWidth',10^3)
legend("normal","VFIB")
title("var")
hold off
```

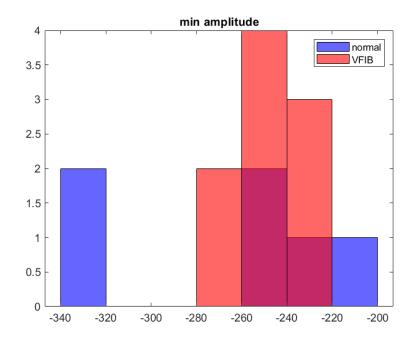


Figure 14: Min Amplitude Comparison for Normal and VFIB Segments

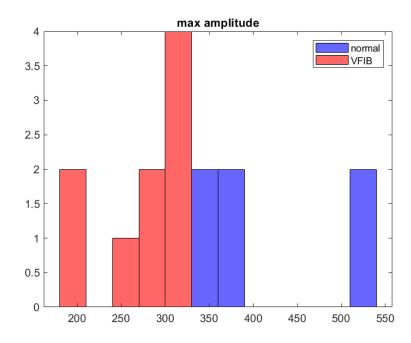


Figure 15: Max Amplitude Comparison for Normal and VFIB Segments

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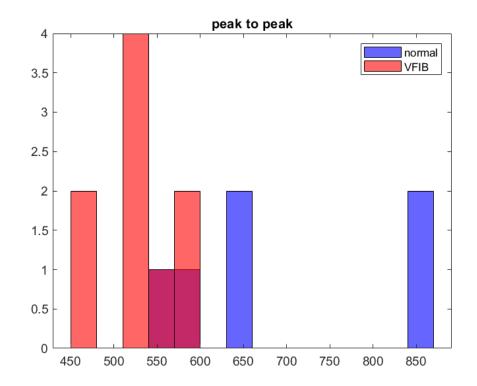


Figure 16: Peak-to-Peak Comparison for Normal and VFIB Segments

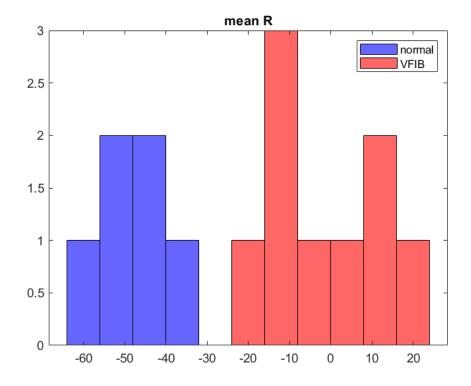


Figure 17: Mean R Comparison for Normal and VFIB Segments

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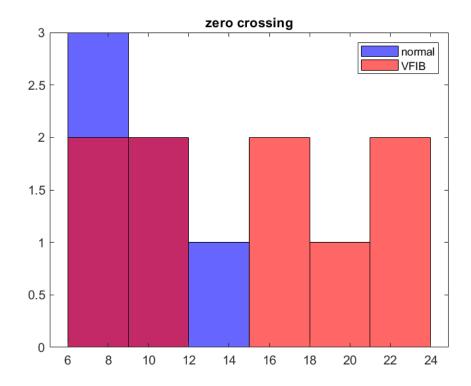


Figure 18: Zero Crossing Comparison for Normal and VFIB Segments

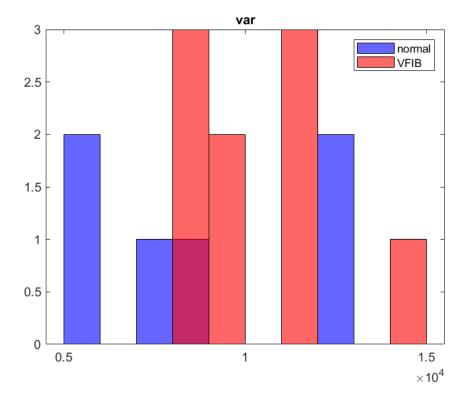


Figure 19: Variance Comparison for Normal and VFIB Segments

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Observations from the feature comparison:

- Criterion 1: Min Amplitude is not suitable for accurate classification.
- Criterion 2: Max Amplitude is suitable for classification, with a threshold set at approximately 325.
- Criterion 3: Peak-to-Peak Value is not suitable for accurate classification.
- Criterion 4: Mean R is suitable for classification, with a threshold set at approximately -28.
- Criterion 5: Zero Crossing is not suitable for accurate classification.
- Criterion 6: Variance is not suitable for accurate classification.

lacksquare Question 10

Considering the results of previous question, select two features and, for each one, complete the va_detect.m function. Obtain and examine the alarm vector (the detection output generated by the selected feature).

```
[alarm_max,t_max] = va_detect(n_422,fs,'max');
[alarm_peak,t_peak] = va_detect(n_422,fs, 'mean-R');
```

■ Question 11

Considering the results of previous question, select two features and, for each one, complete the va_detect.m function. Obtain and examine the alarm vector (the detection output generated by the selected feature).

```
targets = labels((labels(:,1) == 1 | labels(:,1) == 2) , 1) == 2;
2
       outputs_max = alarm_max((labels(:,1) == 1 | labels(:,1) == 2)) == 1;
3
       outputs_peak = alarm_peak((labels(:,1) == 1 | labels(:,1) == 2)) == 1;
4
5
6
       cm1 = confusionmat(targets, outputs_peak);
7
       confusionchart (cm1)
8
9
10
       cm2 = confusionmat(targets, outputs_max);
11
       confusionchart (cm2)
12
13
       targets_all= labels(: , 1);
14
       outputs_max_all= alarm_max+1;
15
       outputs_peak_all = alarm_peak+1;
16
17
       cm1_all = confusionmat(targets_all, outputs_max_all);
18
       confusionchart (cm1_all)
19
       title("max amplitude")
20
21
       figure
22
       cm2_all = confusionmat(targets_all, outputs_peak_all);
23
       confusionchart(cm2_all)
24
       title("peak to peak")
```

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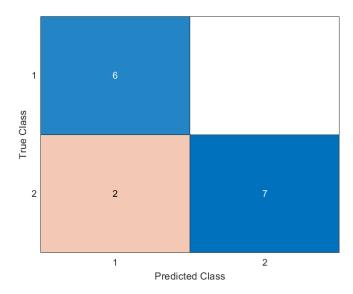


Figure 20: Two class classification based on Max Amplitude confusion matrix

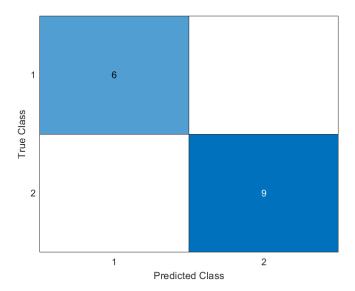


Figure 21: Two class classification based on Mean R confusion matrix

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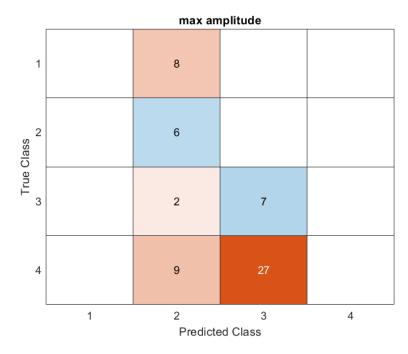


Figure 22: 4 class classification based on Max Amplitude confusion matrix

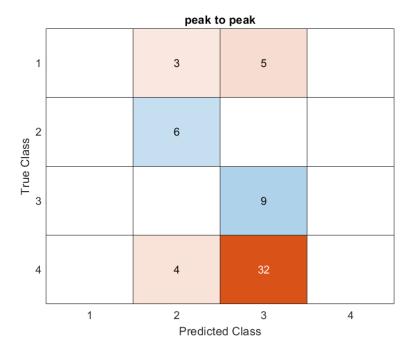


Figure 23: 4 class classification based on Mean R confusion matrix

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Two-Class Classification Based on Max Amplitude

- Accuracy = $\frac{6+7}{6+7+2+0} = 0.86$
- **Sensitivity** = $\frac{6}{6+2} = 0.75$
- Specificity = $\frac{7}{7+0}$ = 1.0

Two-Class Classification Based on Mean R

- Accuracy = $\frac{19+19}{19+19+0+0} = 1.0$
- Sensitivity = $\frac{19}{19+0} = 1.0$
- Specificity = $\frac{19}{19+0} = 1.0$

four-Class Classification Based on Max Amplitude:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 8 to 0.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 9 to 27.

four-Class Classification Based on Mean R:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 3 to 5.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 4 to 32.

Question 12

Do all previous parts for n_424.mat.

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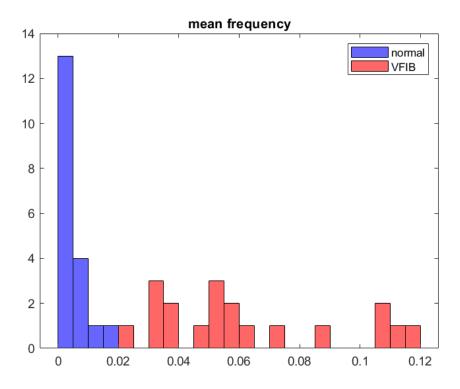


Figure 24: Mean Frequency Comparison for Normal and VFIB Segments

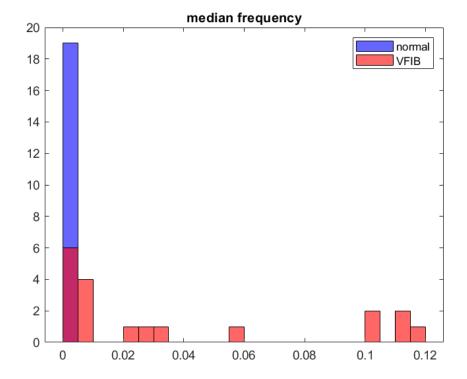


Figure 25: Median Frequency Comparison for Normal and VFIB Segments

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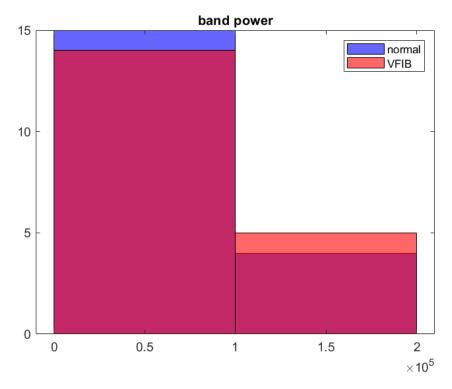


Figure 26: Delta Power in 10-30 Hz Band Comparison for Normal and VFIB Segments

Observations from the feature comparison:

- Criterion 1: Mean frequency is suitable for classification, with a threshold set at approximately 0.02.
- Criterion 2: Median frequency is not suitable for accurate classification.
- Criterion 3: Power in the 10 to 30 Hz band is suitable for classification, with a threshold set at approximately 2×10^6 .

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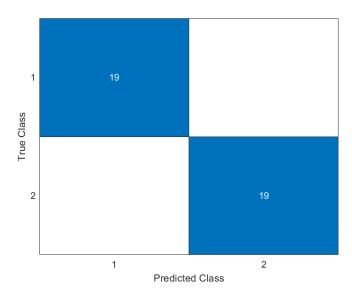


Figure 27: Two class classification based on Mean confusion matrix

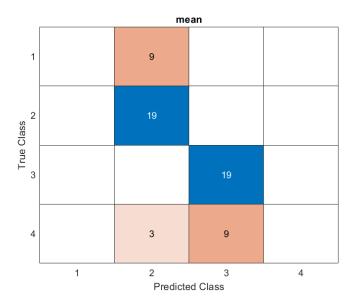


Figure 28: 4 class classification based on Mean confusion matrix

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Two-Class Classification Based on Mean

- Accuracy = $\frac{19+19}{19+19+0+0} = 1.0$
- **Sensitivity** = $\frac{19}{19+0} = 1.0$
- Specificity = $\frac{19}{19+0} = 1.0$

four-Class Classification Based on Mean:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 9 to 0.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 3 to 9.

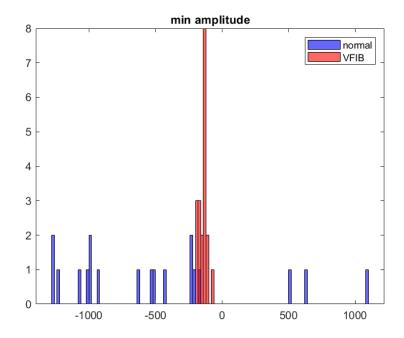


Figure 29: Min Amplitude Comparison for Normal and VFIB Segments

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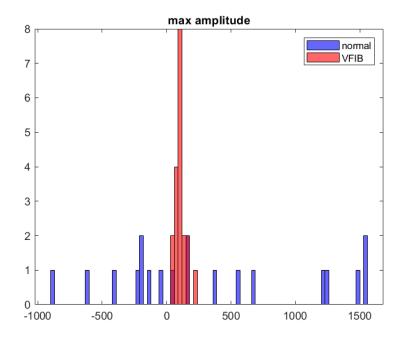


Figure 30: Max Amplitude Comparison for Normal and VFIB Segments

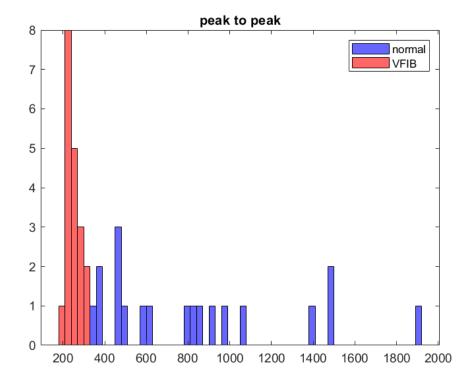


Figure 31: Peak-to-Peak Comparison for Normal and VFIB Segments

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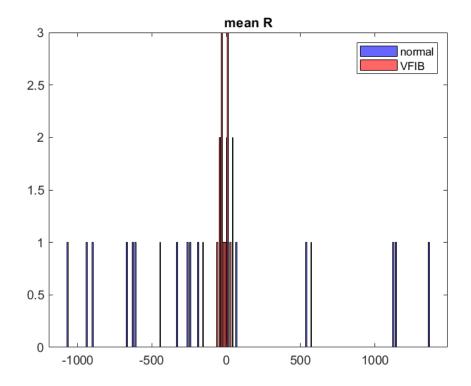


Figure 32: Mean R Comparison for Normal and VFIB Segments

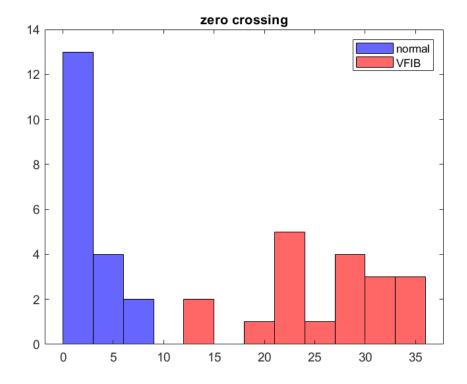


Figure 33: Zero Crossing Comparison for Normal and VFIB Segments

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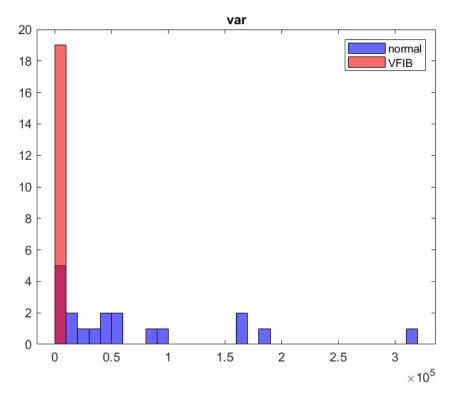


Figure 34: Variance Comparison for Normal and VFIB Segments

Observations from the feature comparison:

- Criterion 1: Min Amplitude is not suitable for accurate classification.
- Criterion 2: Max Amplitude is not suitable for accurate classification.
- Criterion 3: Peak-to-Peak is suitable for classification, with a threshold set at approximately 315.
- Criterion 4: Mean R is not suitable for accurate classification.
- Criterion 5: Zero Crossing is suitable for classification, with a threshold set at approximately 10.
- Criterion 6: Variance is not suitable for accurate classification.

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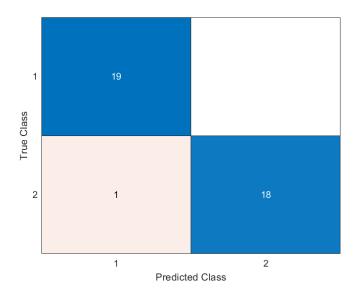


Figure 35: Two class classification based on Peak-to-Peak confusion matrix

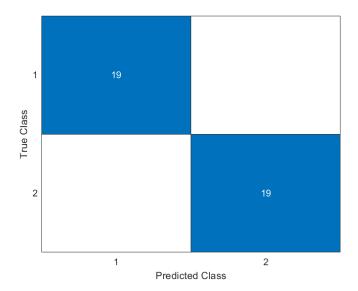


Figure 36: Two class classification based on Zero Crossing confusion matrix

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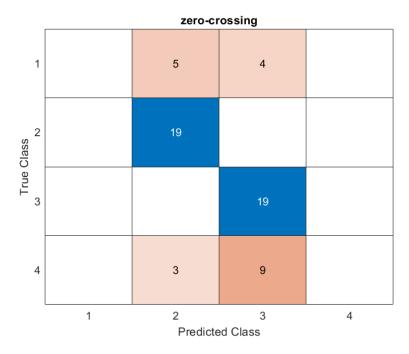


Figure 37: 4 class classification based on Peak-to-Peak confusion matrix

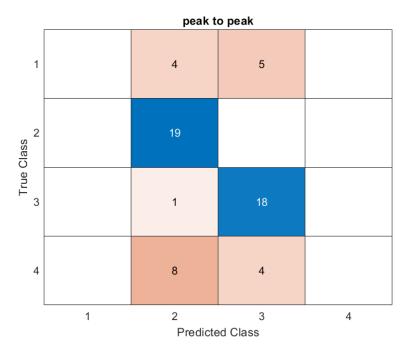


Figure 38: 4 class classification based on Zero Crossing confusion matrix

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Two-Class Classification Based on Peak-to-Peak

- Accuracy = $\frac{19+18}{19+18+1+0} = 0.97$
- **Sensitivity** = $\frac{19}{19+1} = 0.95$
- Specificity = $\frac{18}{18+0} = 1.0$

Two-Class Classification Based on Zero Crossing

- Accuracy = $\frac{19+19}{19+19+0+0} = 1.0$
- Sensitivity = $\frac{19}{19+0} = 1.0$
- **Specificity** = $\frac{19}{19+0} = 1.0$

four-Class Classification Based on Peak-to-Peak:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 5 to 4.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 3 to 9.

four-Class Classification Based on Zero Crossing:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 4 to 5.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 8 to 4.

— Question 13

Compare the best detector obtained for the first dataset with the best detector obtained for the second dataset.

Soloution

The best detector for first dataset is Max Amplitude and the best for the second dataset is Zero-Crossing. The thresholds are different. Each one will have their best performance on different datasets.

— Question 14

Apply the best detector obtained for the first dataset to the second dataset and review the result. Similarly, apply the best detector obtained for the second dataset to the first dataset.

Soloution

We use Zero-crossing for the first data and Max Amplitude for the second one.

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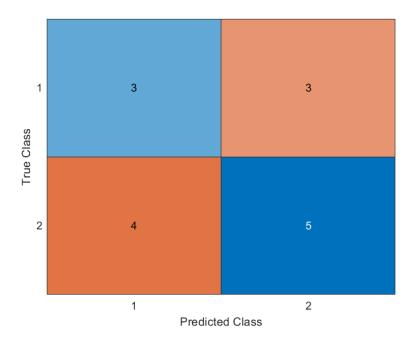


Figure 39: Two class classification based on Zero Crossing confusion matrix for n_422

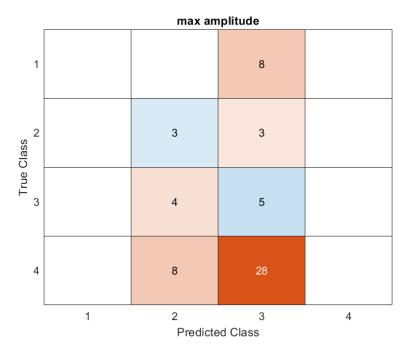


Figure 40: Two class classification based on Zero Crossing confusion matrix for n_422

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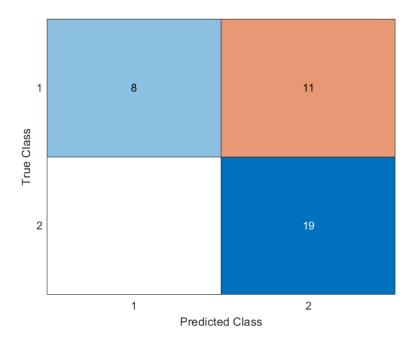


Figure 41: 4 class classification based on Max Amplitude confusion matrix for n_424

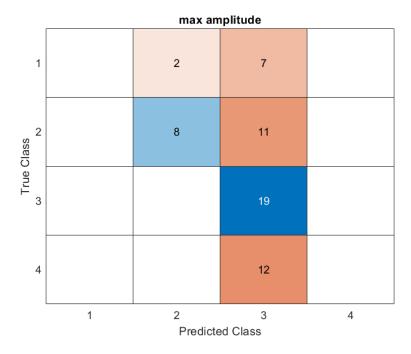


Figure 42: 4 class classification based on Max Amplitude confusion matrix for n_422

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Two-Class Classification Based on Zero Crossing for n_422

- Accuracy = $\frac{3+5}{3+5+3+3} = 0.57$
- Sensitivity = $\frac{3}{3+4} = 0.42$
- Specificity = $\frac{5}{5+4} = 0.55$

Two-Class Classification Based on Max Amplitude for n_424

- Accuracy = $\frac{8+19}{8+19+11+0} = 0.71$
- **Sensitivity** = $\frac{8}{8+0} = 1.0$
- Specificity = $\frac{19}{19+30} = 0.63$

four-Class Classification Based on Zero Crossing for n_422:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 0 to 8.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 8 to 28.

four-Class Classification Based on Max Amplitude for n 424:

The data from the "none" group has been classified into the Normal and VFIB classes with a ratio of 2 to 7.

The data from the "VT" group has been classified into the Normal and VFIB classes with a ratio of 0 to 12.

Question 15

Among the designed detectors, select one as the best detector and apply it to at least one of the other signals. Review and analyze the results. In particular, these files give you an opportunity to observe whether your system produces false alarms in the presence of high noise or remains stable without unnecessary alerts. Does your detector produce false alarms, miss detections (missed detections), or produce both? Under what conditions is your detector more prone to errors?

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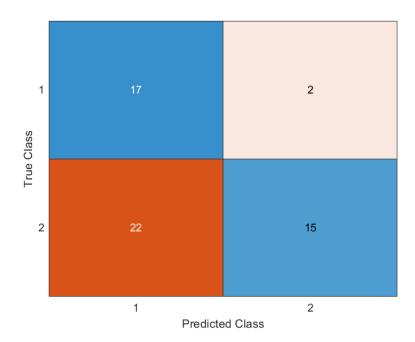


Figure 43: Two class classification based on Zero Crossing confusion matrix for n_426

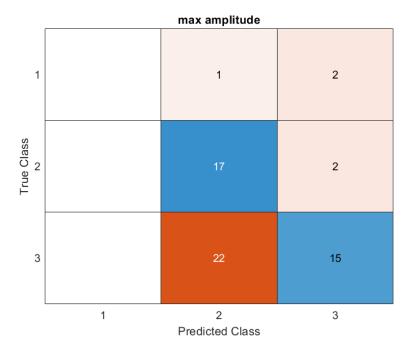


Figure 44: Three class classification based on Zero Crossing confusion matrix for n_426

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I choose Zero-Crossing as the best detector.

Two-Class Classification Based on Zero Crossing for n_426 $\,$

- Accuracy = $\frac{17+15}{17+15+2+22} = 0.6$
- Sensitivity = $\frac{17}{17+22} = 0.43$
- **Specificity** = $\frac{15}{15+2} = 0.88$

Based on the confusion matrix, we can see our detector is not robust to noise. It also can not detect the VT and Noise.

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