

Intensity based Image Registration

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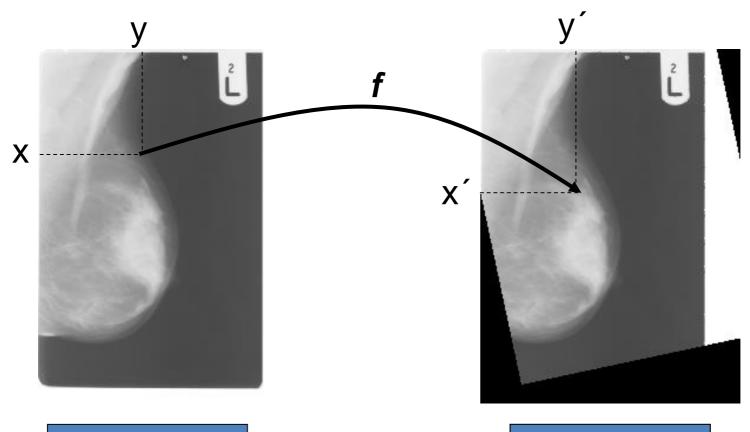




Image Registration. Overview

Find the transformation or mapping function f

$$T(x', y') = R(f(x, y))$$





Reference

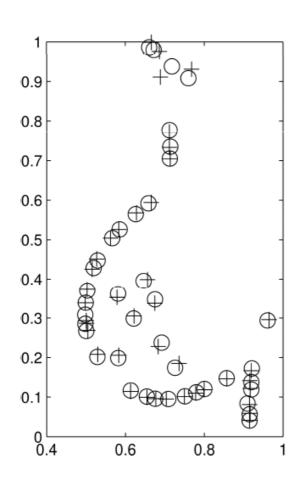
Target



Image Registration. Components

Classification:

Intensity based vs feature based (aka dense vs sparse)



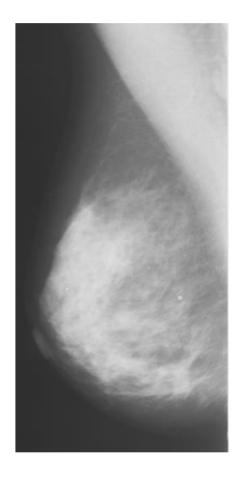


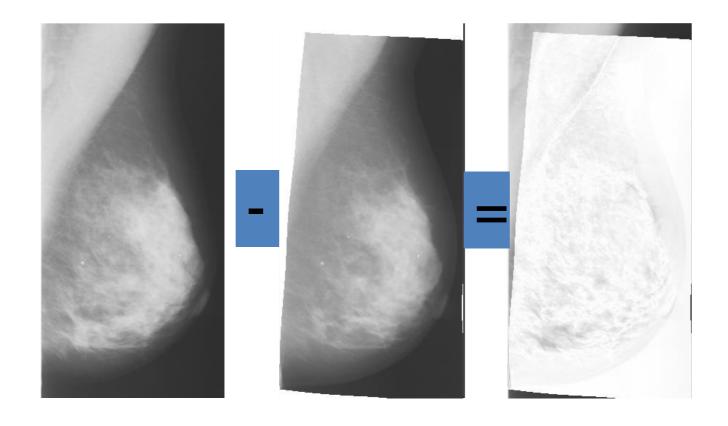




Image Registration. Classification

Classification:

Rigid vs non-rigid (aka deformable, local)

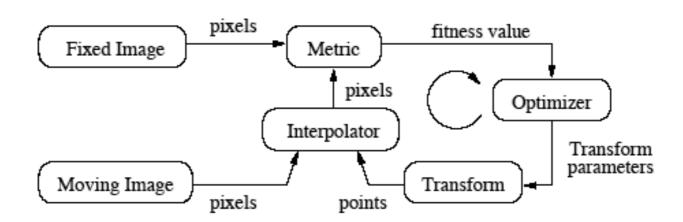






Components

- Transform: allowed movement of the moving image, depends on some parameters.
- Metric: Measure of similarity between fixed and moving.
- Interpolator: Determines the pixel intensity given the position and neighbour pixels.
- **Optimizer:** finds the best metric value with respect to the transformation parameters.







Transform

- Many different classifications
 - Global vs Local
 - Parametric vs Non-parametric
- Global: all pixels suffer the "same" transformation.
 - Rigid: Rotation and translation
 - Similarity: Rigid + Scaling
 - Affine: Similarity + Shearing and tearing (keeps parallelism)
 - Perspective



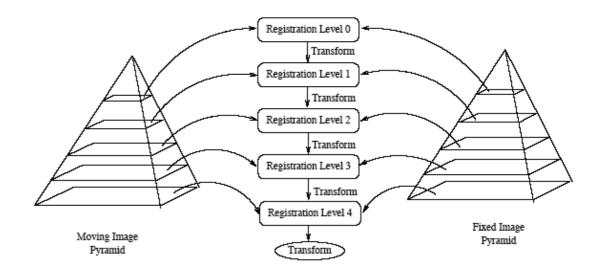


Transform

- Local: pixels can move independently at a local level.
 - Thin Plate Splines. Based on point correspondence and spline interpolation
 - B-Splines (Free-Form deformations). Deform grids of points based on B-spline interpolation.
 - Demons, Finite Element Modelling, Poly Rigid, Local Affine, ...

Variations

- Global + Local
- Multi-resolution







Global Transform

Rigid

$$f_x(x,y) = x\cos\phi + y\sin\phi + t_x$$

$$f_y(x,y) = -x\sin\phi + y\cos\phi + t_y$$

Affine

$$f_x(x,y) = a_x x + a_y y + t_x$$

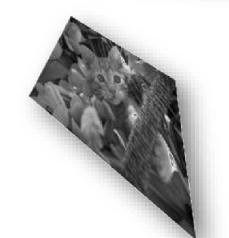
$$f_y(x,y) = b_x x + b_y y + t_y$$



$$f_x(x,y) = \frac{a_x x + a_y y + t_x}{c_x x + c_y y + 1}$$
$$f_y(x,y) = \frac{b_x x + b_y y + t_y}{c_x x + c_y y + 1}$$









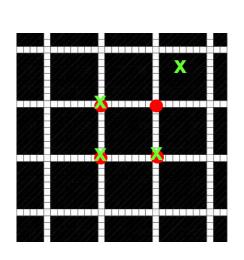
Local (non-rigid) Transformations

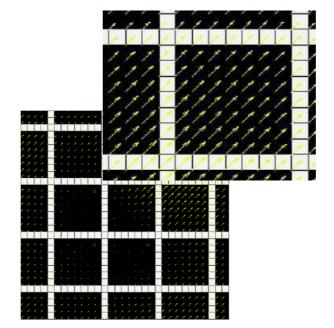
Thin Plate Splines

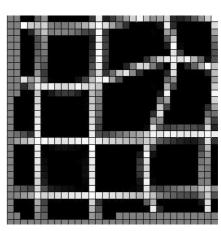
$$\iint_{R^2} \left(\left(\frac{\partial^2 f}{\partial x^2} \right)^2 + 2 \left(\frac{\partial^2 f}{\partial x \partial y} \right)^2 + \left(\frac{\partial^2 f}{\partial y^2} \right)^2 \right) dx dy \qquad f_x(x, y) = a_x x + a_y y + t_x + \sum_{i=1}^N w_i U(|\vec{p}_i - (x, y)|)$$

$$f_y(x, y) = b_x x + b_y y + t_y + \sum_{i=1}^N w_i U(|\vec{p}_i - (x, y)|)$$

$$U(r) = r^2 \log r^2$$











Local (non-rigid) Transformations

B-Splines grid (Free-form deformations)

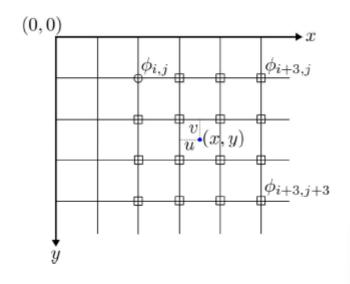
$$\mathbf{T}_{local}(x, y, z) = \sum_{l=0}^{3} \sum_{m=0}^{3} \sum_{n=0}^{3} B_{l}(u)B_{m}(v)B_{n}(w)\phi_{i+l, j+m, k+n}$$

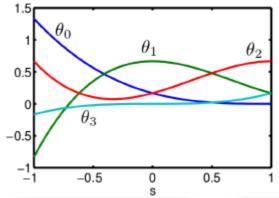
$$B_0(u) = (1 - u)^3/6$$

$$B_1(u) = (3u^3 - 6u^2 + 4)/6$$

$$B_2(u) = (-3u^3 + 3u^2 + 3u + 1)/6$$

$$B_3(u) = u^3/6.$$





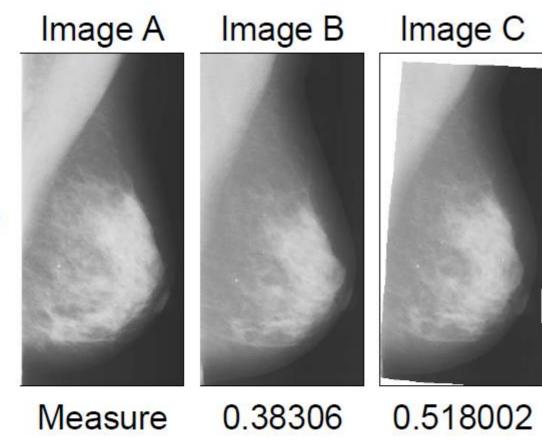








How similar two images are?







- Measure the similarity between images
- Definition of a metric between image A and B (C).

$$R1$$
) $d(\mathbf{A}, \mathbf{B}) > 0$

$$R2$$
) $d(\mathbf{A}, \mathbf{B}) = 0$ iff $\mathbf{A} = \mathbf{B}$

$$R3)$$
 $d(\mathbf{A}, \mathbf{B}) = d(\mathbf{B}, \mathbf{A})$

R4)
$$d(\mathbf{A}, \mathbf{B}) \le d(\mathbf{A}, \mathbf{C}) + d(\mathbf{C}, \mathbf{B})$$

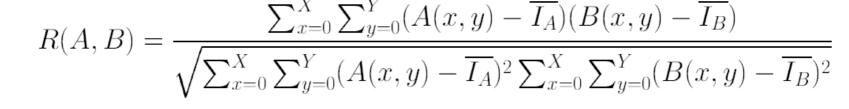




Simple Intensity difference (Root mean squared)

$$RMS(A,B) = \frac{1}{N} \sqrt{\sum_{x=0}^{X} \sum_{y=0}^{Y} (A(x,y) - B(x,y))^2}$$

- Normalised cross correlation
 - Correlation between pixels in both images.
 - High values denote high similarity
 - Intensity, gradient, etc.







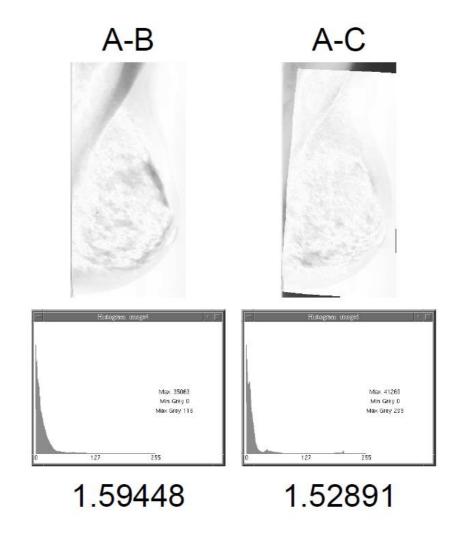
- Entropy related measures
 - Mutual information
 - Entropy of the difference image
 - Low values, low entropy, hence similar images?

$$S_{AB} = \sum_{x=0}^{X} \sum_{y=0}^{Y} A(x, y) - sB(x, y)$$
$$H(S_{AB}) = -\sum_{i=0}^{I} p(i) \log(p(i))$$





Entropy of the difference image







Mutual Information

$$C(A,B) = \sum_{i=0}^{I} \sum_{j=0}^{J} p_{AB}(i,j) \log \frac{p_{AB}(i,j)}{p_{A}(i)p_{B}(j)}$$

$$= H(A) + H(B) - H(A, B)$$

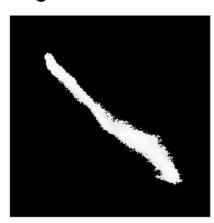
Joint histogram



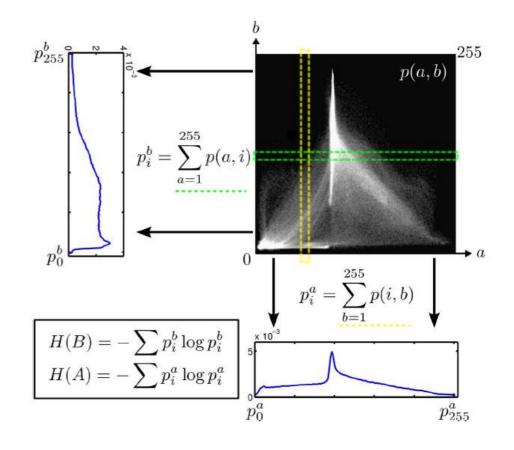
Before 0.38306

Universitat

de Girona

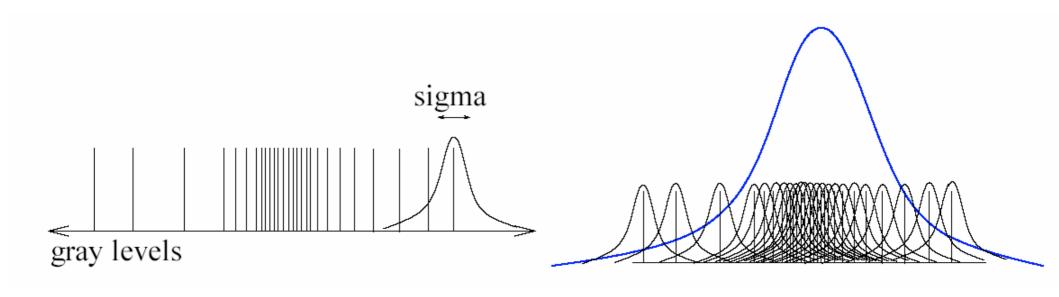


After 0.518002





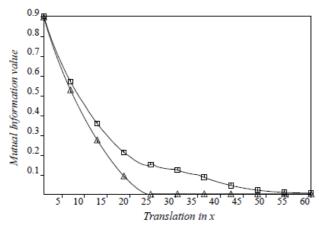
- How to estimate the histogram?
- Has to be a continous distribution!
- Parzen Window estimation

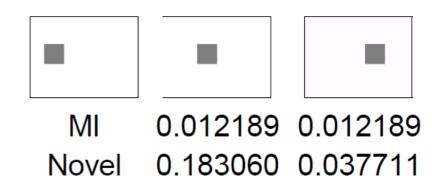






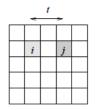
Variations: Non-overlapping MI.

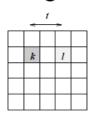




- Incorporate spatial information into MI
- Pixel pairs instead of single pixels (GLCM)

Image A Image B





| A-B | A-C |
|----------|----------|
| 0.335626 | 0.441571 |





- Mathematically express the human perception of similarity
- Does not always work!

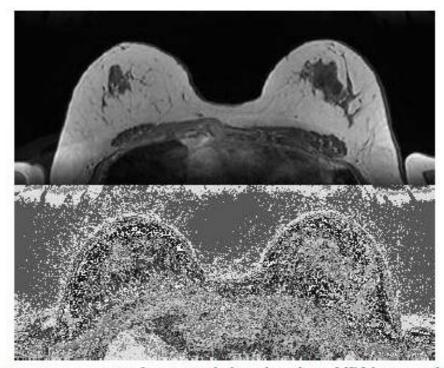


Figure 1. Example of image intensity swapping for an axial slice though an MRI breast volume. Pixel intensity values in the original image a are binned and arbitrarily rearranged to give image b. The mutual information (MI) between these two images is maximal (here, for 64 bins, MI=6) and the images may be regarded as being identical.





- Mathematically express the human perception of similarity
- Does not always work!

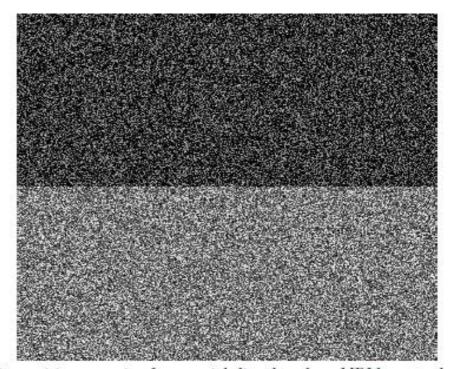


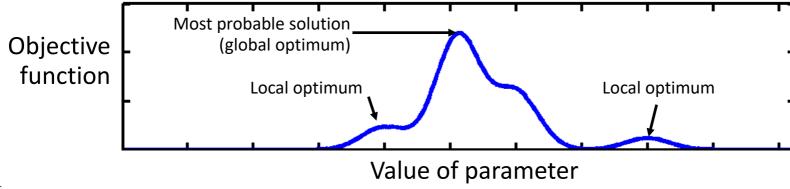
Figure 2. Example of intensity position swapping for an axial slice though an MRI breast volume (1a). The pixel positions are arbitrarily rearranged in space. These images have the same marginal entropy as Figure 1a. Figure 2b has had the intensity values swapped as in Figure 1b. Again, the mutual information (MI) between these two images is maximal (here, for 64 bins, MI=6) and the 'images' may be regarded as being identical





Optimizer

- Finds the transformation parameters that maximises a similarity measure
- Gradient descent algorithms
- Usually need to specify the gradient of the metric with respect to the transformation parameters



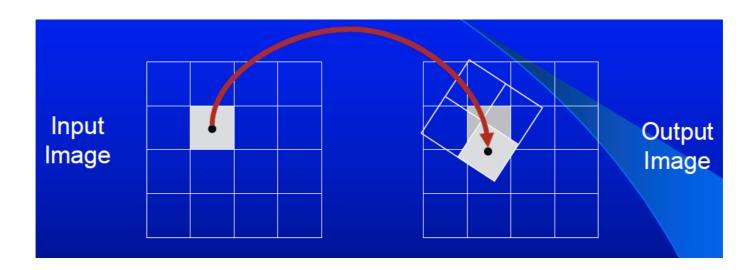




Mapping

Forward mapping

- Input image pixel is mapped onto the output image
- Output pixels with more than one hit: overlap
- Value must be accumulated from overlapping pixels
- Output pixels with no hits: hole

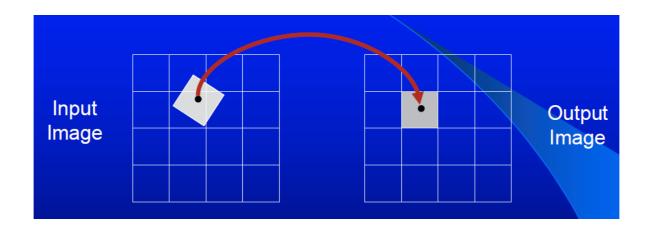






Mapping

- Inverse mapping
 - Output pixels are mapped back onto the input image
 - Output pixel value must be interpolated from a neighborhood in the input image
 - Scheme avoids any holes and overlaps in the output image because all pixels are scanned sequentially







Interpolator

Transforming the image

```
for y=1...n_y % loop over rows for x=1...n_x % loop over columns x' = f_x(x,y) \text{ % transform} y' = f_y(x,y) if 1 \le x' \le n_x, & 1 \le y' \le n_y, then % voxel in range newB(x,y) = B(x',y')%assign re-sampled value end % voxel in range end end
```

- What if x',y' are not integers?
- Inverse transform





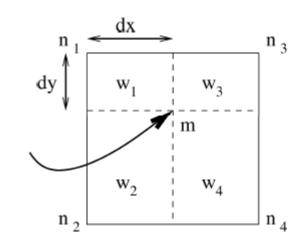
Interpolator

- Transformed coordinates are usually non-integers, $m=(x^\prime,y^\prime)$
- Assign the intensity of
 - Nearest Neighbour

$$B(m) = B(\min_{\forall i}(d_E[m, n_i]))$$

Linear interpolation

$$B(m) = \sum_{i} w_i B(n_i)$$



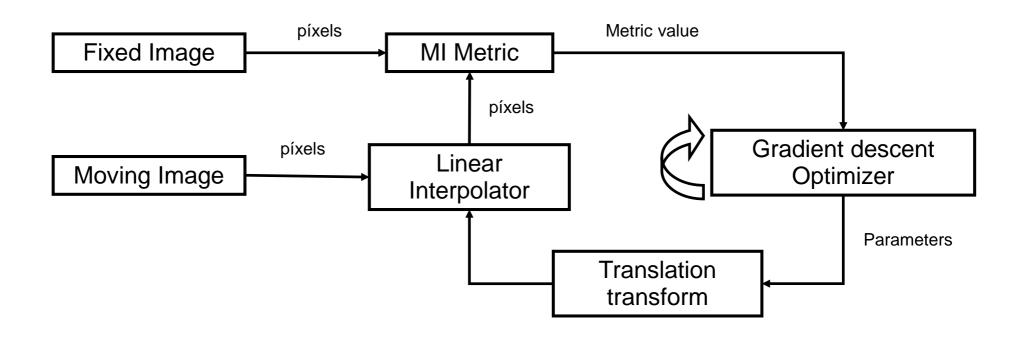
$$w_1 = (1 - dx)(1 - dy)$$
 $w_2 = (1 - dx)dy$ $w_3 = dx(1 - dy)$ $w_4 = dxdy$

Cubic Interpolation





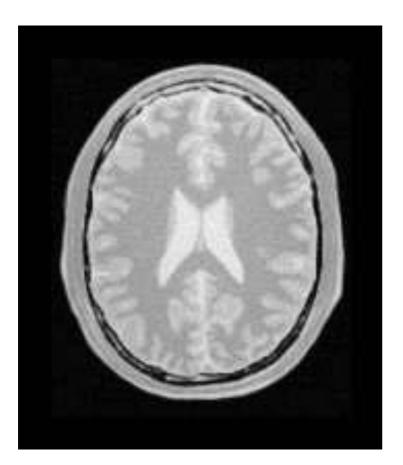
Hello world Registration example

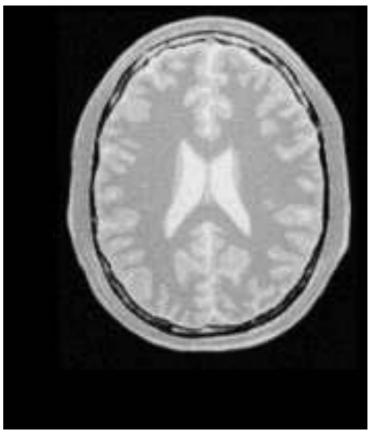






Hello world input

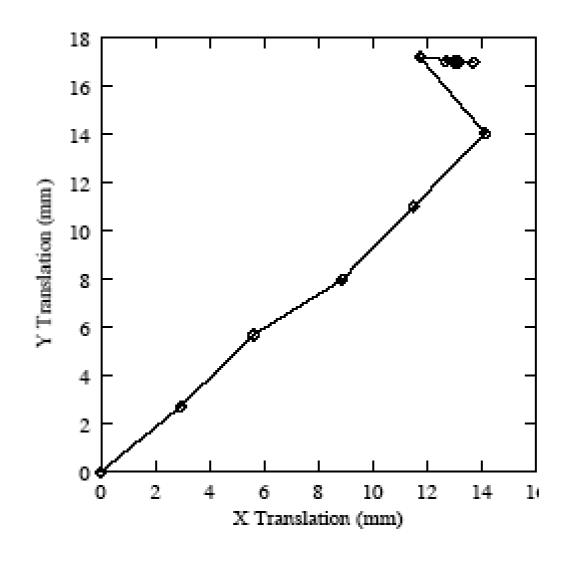








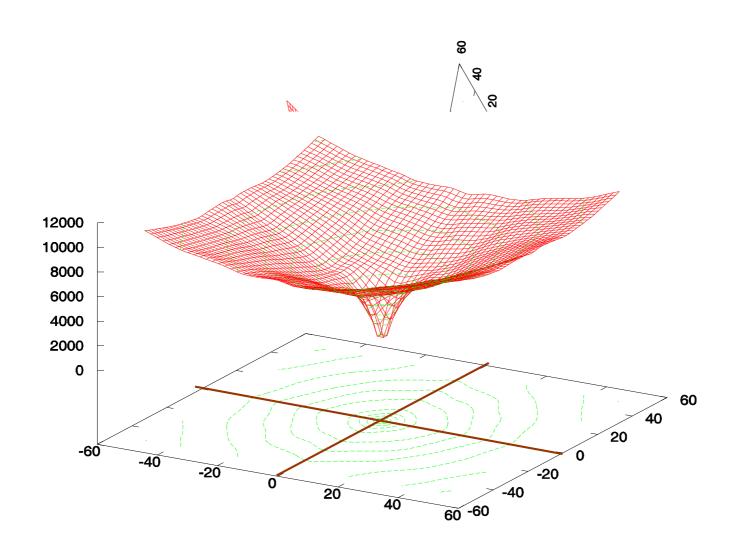
X & Y translation vs. time







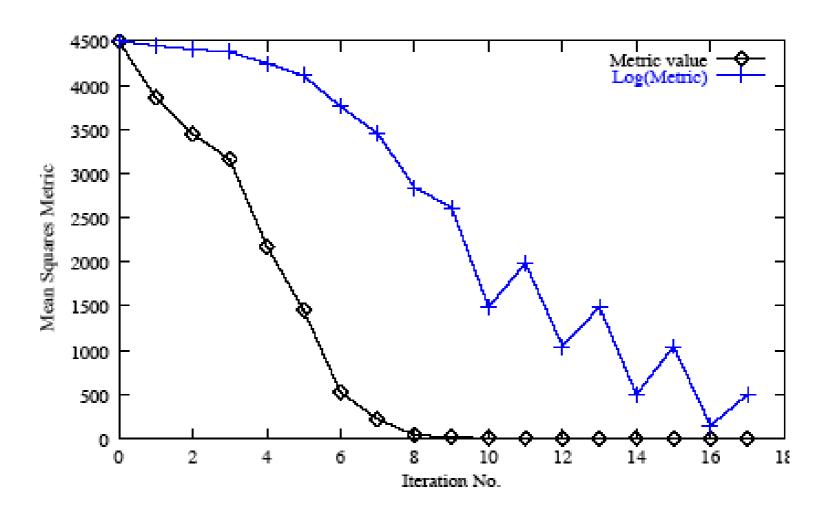
X & Y translation vs. time







Metric vs. time







Gradient Descent

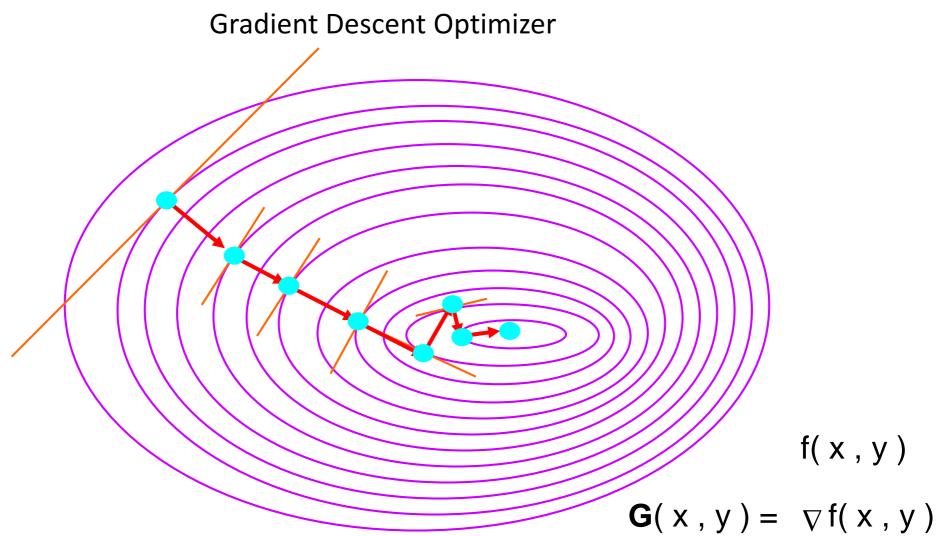
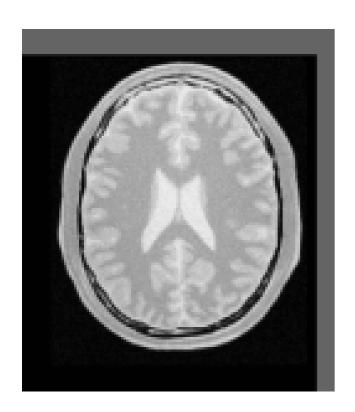
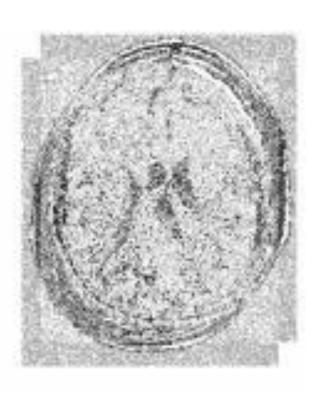






Image comparison

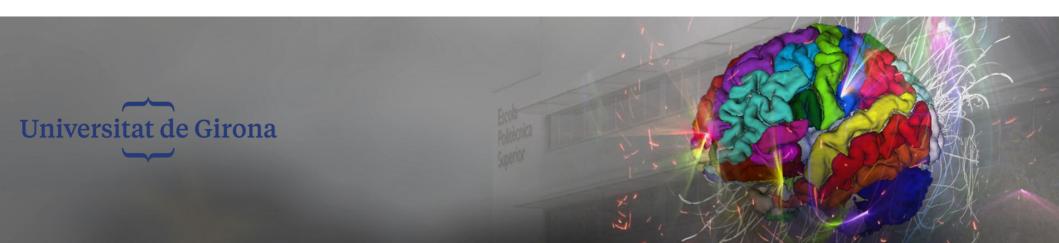








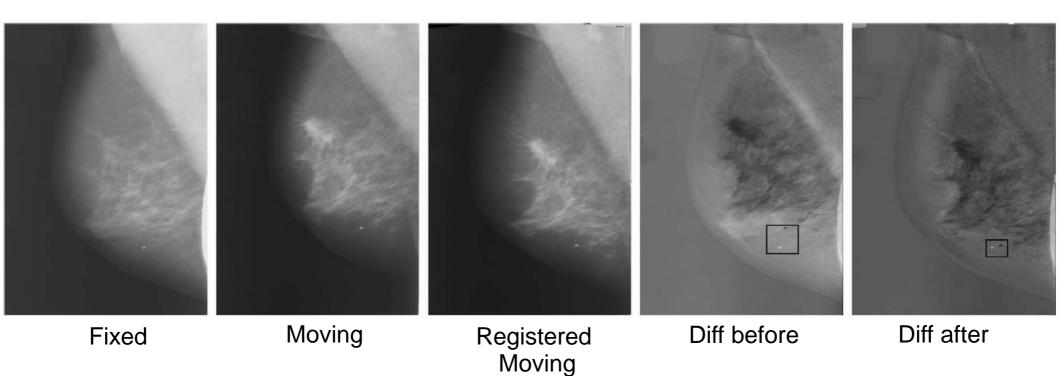
Evaluating your registration





How to evaluate?

You have developed your image registration algorithm... now what?







Validation of algorithms

- Technical validation
 - Accuracy, Robustness, speed, reliability
- Clinical Validation
 - Is it useful for the doctors?
 - Does it help to improve diagnosis/treatment?
- Comercial System
 - FDA Approval





Evaluation criteria

- Robustness
 - Variability for starting conditions of the registration
 - Noise, allowed misregistration, landmark error, etc.
- Consistency
- Visual assessment
 - Subtraction images
 - Checkerboard, overlay
- Quantitative analysis
 - Landmark error
 - Simulated deformations
 - Similarity metrics.
- Ground Truth!?

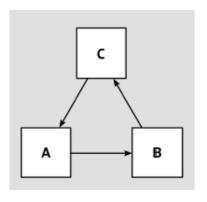




Consistency

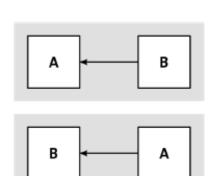
Apply various registration in order to evaluate the consistency.

$$T_{AB}(T_{BC}(T_{CA}(x))) = I(x) = x$$



- Forward /inverse consistency
 - Bijectivity/diffeomorphic registration









Visual Assessment

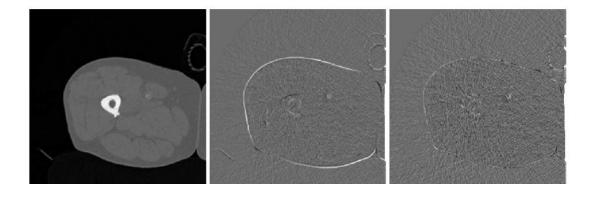
- Qualitative assessment. Observer opinion.
- Intra inter observer variability!
- Subtraction images
- Overlay
 - Checkboard
 - Contours
 - Colors



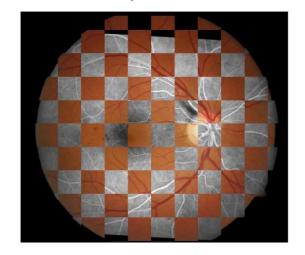


Visual Assessment

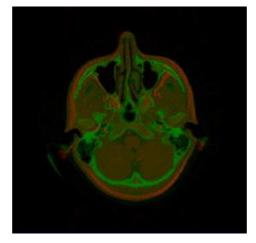
- Subtraction images
 - Absolute?



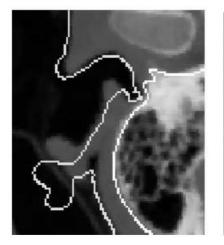
Overlay



Checker board



Color (R & G)



Contour







Visual Assessment

Example

Observer study

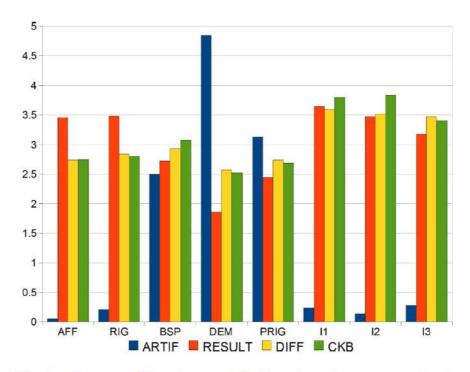


Fig. 4. Summary of the observer study. Bars show observer perception, in all cases higher means better except for the number of artifacts (ARTIF) were lower means better. AFF = affine, RIG = rigid, BSP = B-Splines FFD, DEM = Demons, PRIG = polyrigid, I1 = MR BSP, I2 = AFF + BSP, I3 = MR AFF + MR BSP.

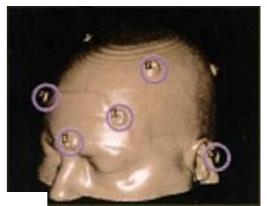
Y.Díez, A.Oliver, X.Lladó, J.Freixenet, J.Martí, J.C.Vilanova, and R.Martí. Revisiting intensity-based image registration appplied to mammography. IEEE Trans. on Information Technology in BioMedicine, 15(5), pp 716-725, 2011.

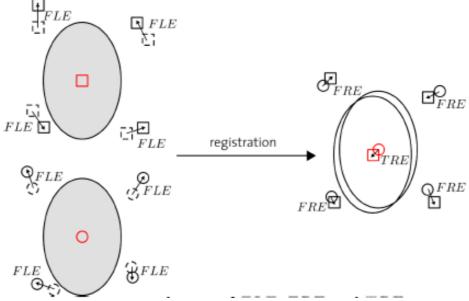




Errors

- Fiducial Localization Error (FLE)
- Fiducial Registration Error (FRE)
- Target Registration Error (TRE)



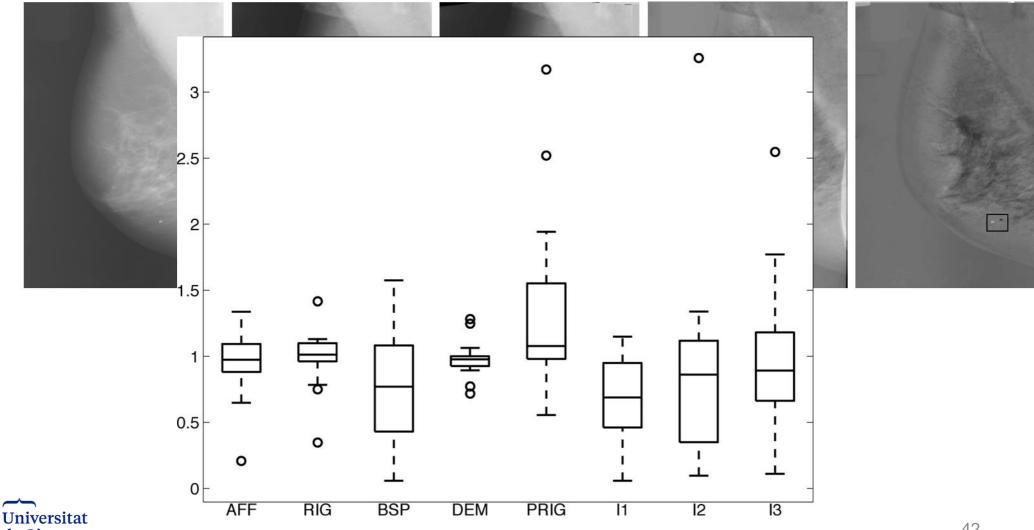






Errors. example

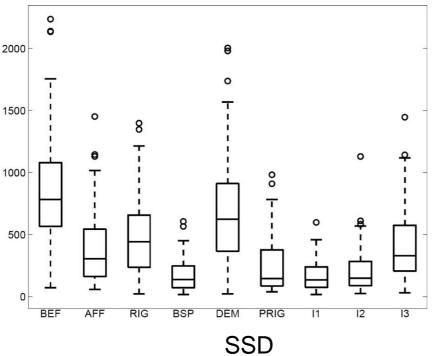
TRE: Computing error after registration between microcalcifications.

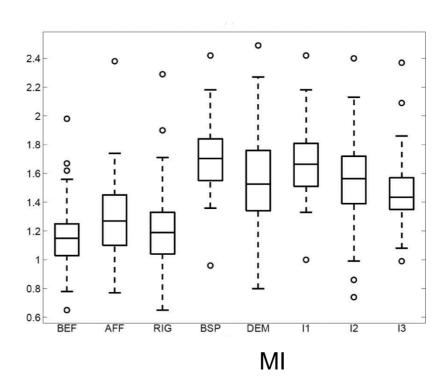




Similarity metrics

- Metric comparison
 - A higher metric DOES NOT always mean better registration



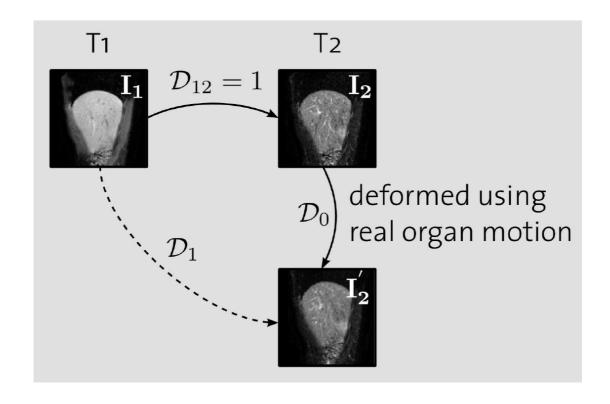






Synthetic / Simulated models

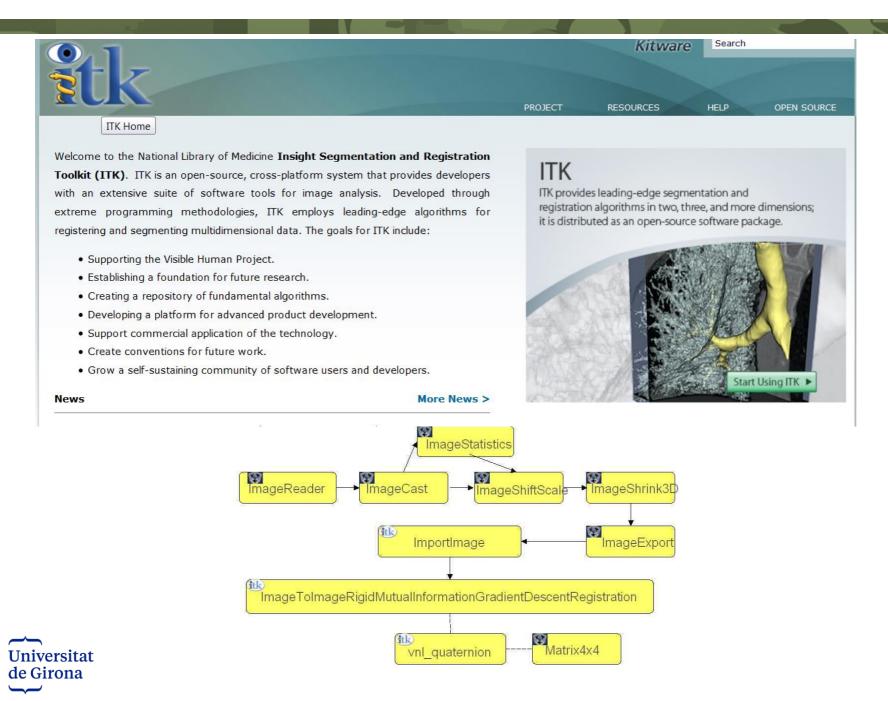
- Difficulty of obtaining the ground truth
- Synthetic/Simulated examples
- Simulate deformation and recover it with IR.







ITK & Image registration





Matlab & Image registration



The immegconfig function makes it easy to pick the correct optimizer and metric configuration to use with immegister. These two images have different intensity distributions, which suggests a multimodal configuration.

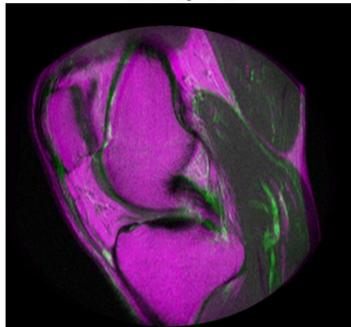
```
[optimizer,metric] = imregconfig('multimodal');
```

The distortion between the two images includes scaling, rotation, and (possibly) shear. Use an affine transformation to register the images.

It's very, very rare that immegister will align images perfectly with the default settings. Nevertheless, using them is a useful way to decide which properties to tune first.

```
movingRegisteredDefault = imregister(moving, fixed, 'affine', optimizer, metric);
f3 = figure;
imshowpair(movingRegisteredDefault, fixed);
figure(f3);
title('A: Default registration');
```

A: Default registration







Software & Libraries

Niftyreg

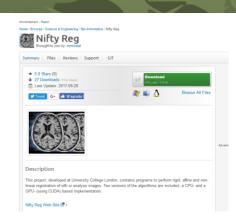
https://sourceforge.net/projects/niftyreg/

ANTS

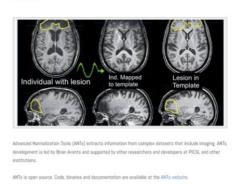
http://picsl.upenn.edu/software/ants/

Elastix

http://elastix.isi.uu.nl/



ANTS







MAIA

ITK

- Getting Started
 - http://www.itk.org/CourseWare/Training/GettingStarted-I.pdf
 - http://www.itk.org/CourseWare/Training/GettingStarted-III.pdf
 - Example code: ImageRegistration1.cxx
- Software Guide http://www.itk.org/ltkSoftwareGuide.pdf





To know more...

- Insight into Images: Principles and Practice for Segmentation, Registration and Image Analysis, Terry S. Yoo (Editor)
- Handbook of Medical Imaging: Processing and Analysis, Isaac Bankman (Editor)
- Fundamentals of Medical Imaging, P. Suetens, Cambridge University Press 2002
- A. Melbourne, G. Ridgway, D. J. Hawkes. Image Similarity Metrics in Image Registration. CMIC, UCL London.
- Medical Image Analysis, A. Dhawan, Wiley 2003
- ITK Software Guide (<u>www.itk.org</u>)

