

## INTRODUCTION

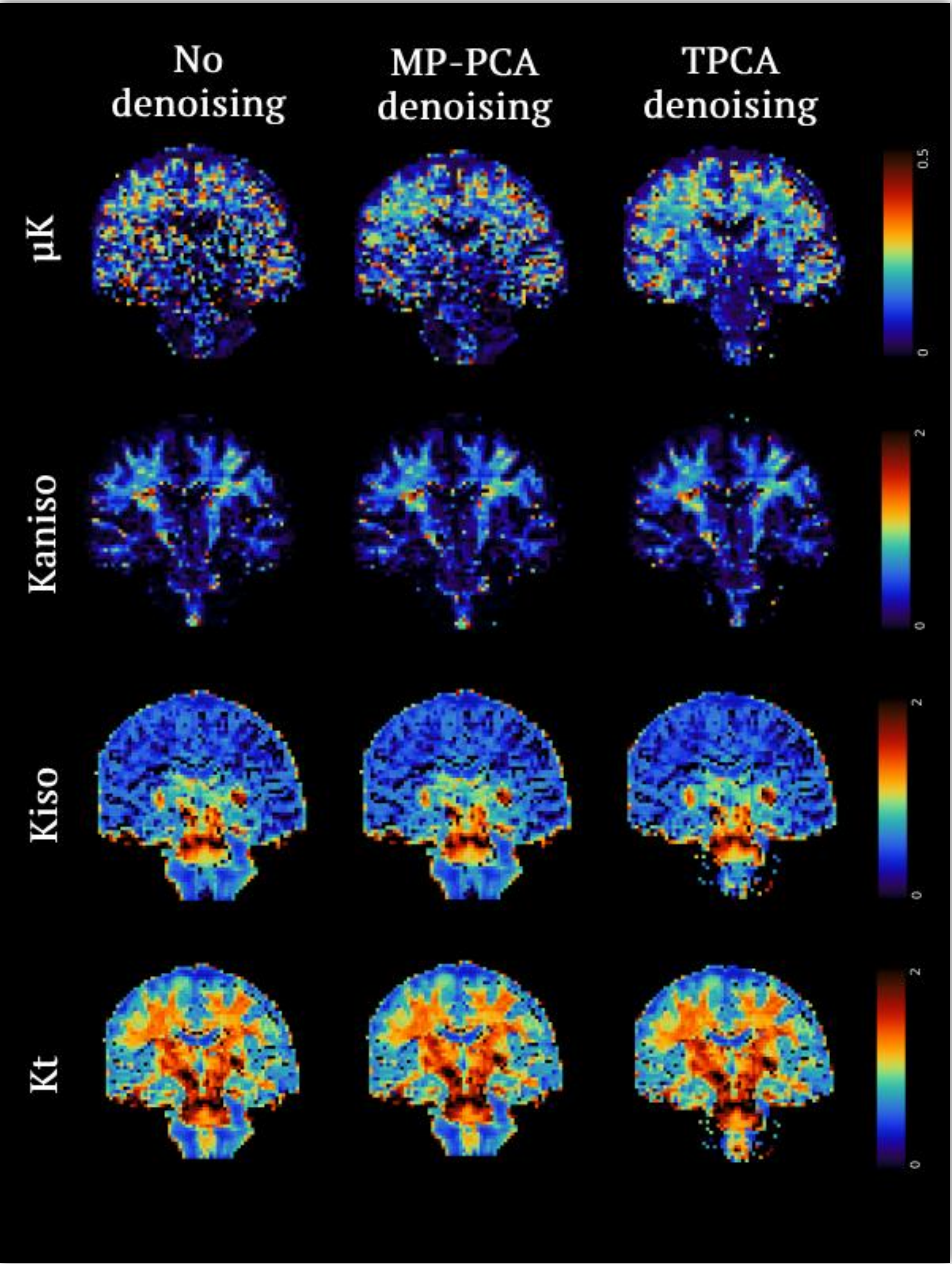
- Correlation Tensor Imaging (CTI)<sup>1</sup>** (**K**: Kurtosis)
- Promising preclinical<sup>2</sup> & human<sup>3</sup> evidence
- Human acquisitions ~ 50min  
→ Limited clinical feasibility → **Acceleration** is critical
- Acceleration → SNR losses → **Denoising is critical**
- This work compares 3 denoising pipelines on human CTI data at 3T:**
  - P1: No Denoising (Reference)*
  - P2: Marčenko-Pastur PCA (**MP-PCA**)<sup>4</sup>*
  - P3: Threshold PCA (**TPCA**)<sup>5</sup>*

$$\mathbf{K}_{\text{iso}} + \mathbf{K}_{\text{aniso}} + \mu\mathbf{K} = \mathbf{K}_{\text{T}}$$

## METHODS

- Population & MRI Acquisition:**
  - CTI data of 8 healthy young volunteers, 3T MRI<sup>3</sup>
- Preprocessing and CTI:**
  - Denoising:** *P1 (None), P2 (MP-PCA), P3 (TPCA)*
  - Gibb's ringing (MRtrix3)*
  - Geometric distortions and eddy currents (FSL),*
  - Signal drift<sup>6</sup>, Bias field (MRtrix3)*
- Statistical Analysis:**
  - Denoising Performance:**
    - Mean Values of CTI metrics
    - Within-ROI variability of CTI metrics
    - % CTI fit fails (biologically implausible)
  - Pipeline Effects:** Friedman → Wilcoxon's + FDR correction

## RESULTS



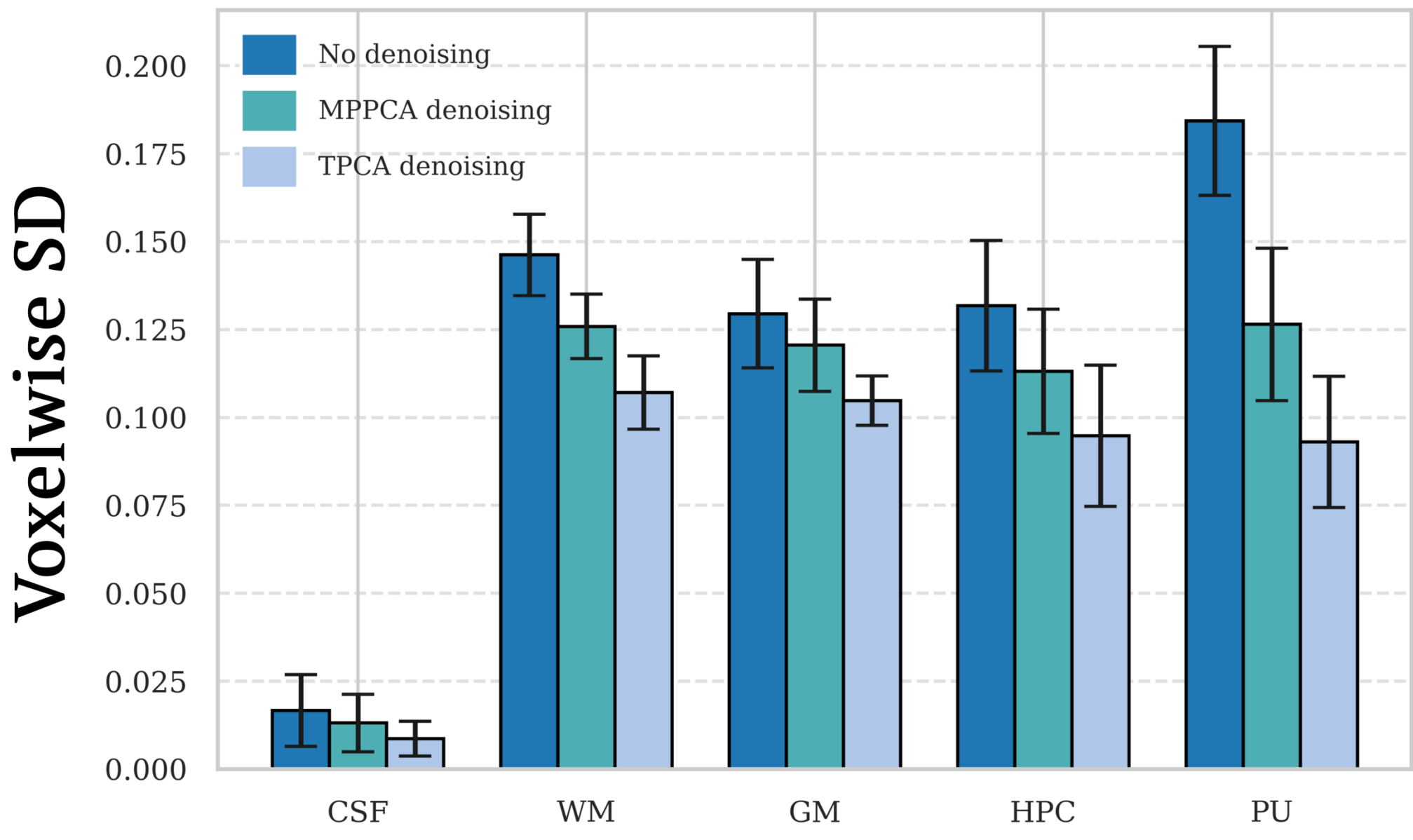
**Figure 1.** Single subject CTI derived maps of microkurtosis ( $\mu\mathbf{K}$ ), anisotropic kurtosis (Kanis), isotropic kurtosis (Kiso), and total kurtosis (Kt) across denoising pipelines.

## DISCUSSION

- PCA denoising does not affect mean CTI ROI values**
- But, both PCA methods reduce CTI variability within ROIs, especially in  $\mu\mathbf{K}$ :**
  - Lower voxelwise standard deviation ( $p < 0.01$ )
  - Lower biologically implausible fits ( $p < 0.01$ )
- TPCA outperforms MP-PCA (WM & GM regions)**
- CSF: Strongest difference in % negatives between the P1, P2 and P3

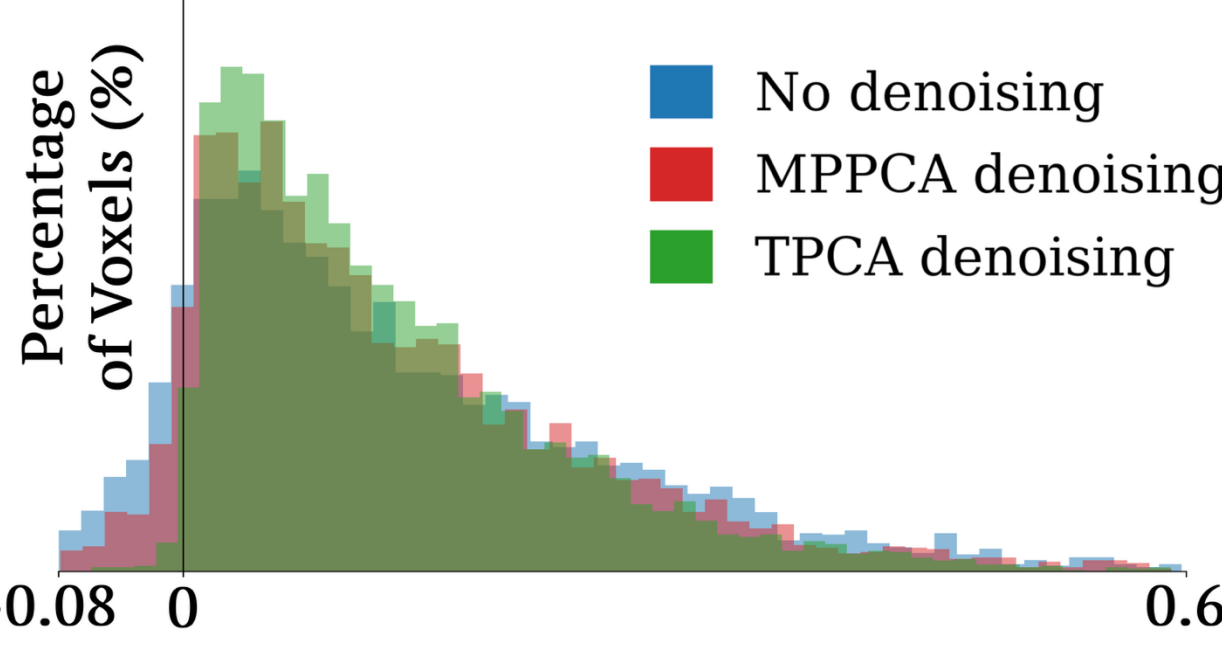
a)

### Voxelwise Variability - $\mu\mathbf{K}$

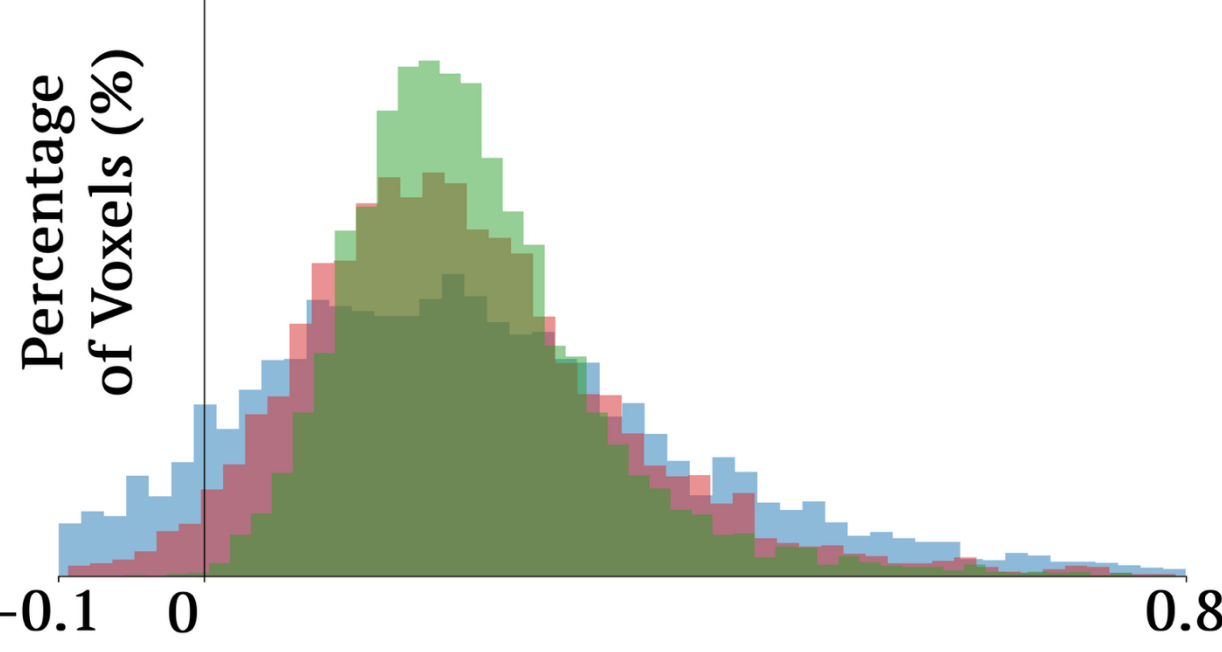


b)

### $\mu\mathbf{K}$ values for HPC



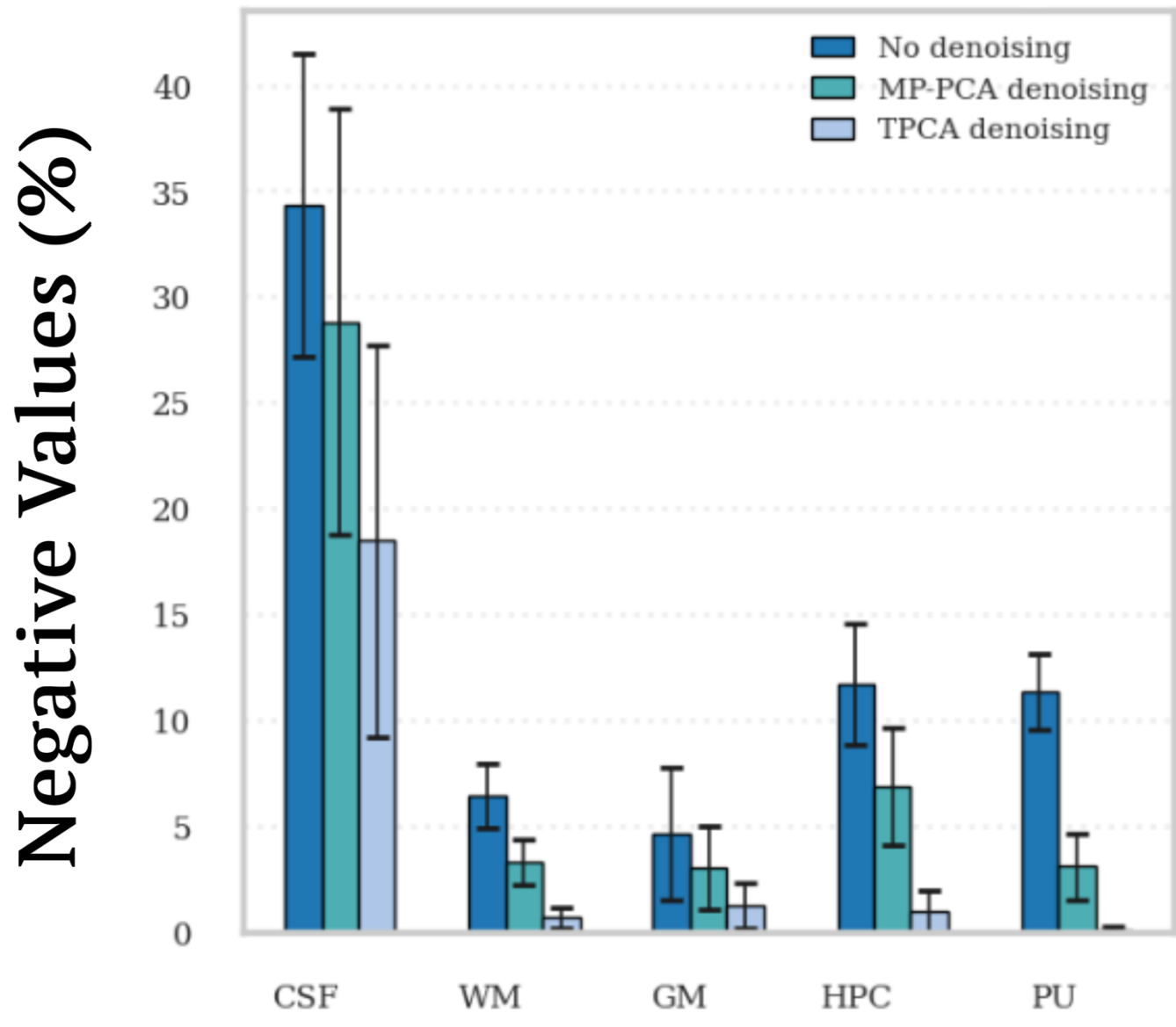
### $\mu\mathbf{K}$ values for PU



**Figure 2.** Denoising reduces  $\mu\mathbf{K}$  variability. (a)  $\mu\mathbf{K}$  variability drop ( $P1 > P2 > P3$ ) across regions. (b)  $\mu\mathbf{K}$  distributions in HPC (top) and PU (bottom).

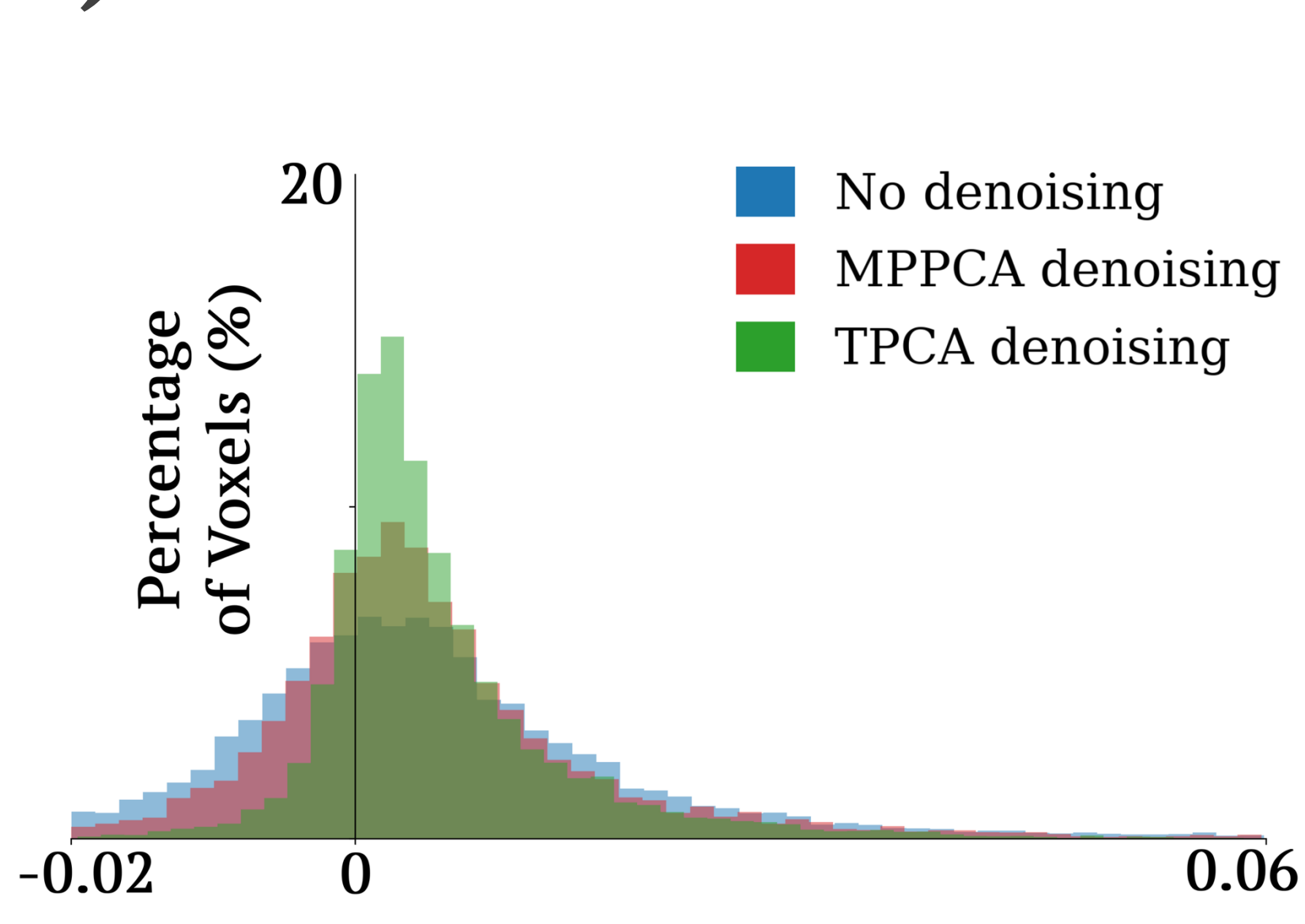
a)

### Percentage Negative - $\mu\mathbf{K}$



b)

### $\mu\mathbf{K}$ values for CSF



**Figure 3.** Denoising reduces % negative  $\mu\mathbf{K}$  fits. (a)  $P1 > P2 > P3$  across regions. (b) CSF  $\mu\mathbf{K}$  distribution.

## CONCLUSION

- Denoising Performance:**
  - P3 (TPCA) > P2 (MP-PCA) > P1 (No Denoising)**
  - Correcting for spatial autocorrelations (TPCA) improves CTI accuracy**
- Strongest Improvement:**
  - CTI Metric:  $\mu\mathbf{K}$ , Brain Regions: CSF, HPC, Pu
- Future Directions:**
  - Add Rician bias correction
  - Acquisition of CTI data with an accelerated (~12m) protocol
  - Test-retest reproducibility of current results

